Revisiting the Stimulation-Rate-Dependent Pattern Mismatch Negativity

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Abstract

How does the brain process and represent successive sound in close temporal proximity? By investigating mismatch negativity (MMN) components, prior research (Sussman & Gumenyuk, 2005; Sussman, Ritter & Vaughan, 1998) has suggested that temporal proximity plays an important role in how sounds are represented in auditory memory. Here, we investigate how predictability affects the election of mismatch negativity components in auditory sequences consisting of two tones (frequent tone A = 440 Hz, rare tone B = 494 Hz, fixed SOA 100 ms). In the predictable condition, tones are presented in a fixed order whereas in the unpredictable condition, standards and deviants are presented in a pseudo-random order. We expect to find that B tones in the unpredictable condition will elicit a significant MMN while B tones in the predictable conditions will not. A repeating five-tone pattern was presented at several stimulus rates (200, 400, 600, and 00 ms onset-to-onset) to determine at what temporal proximity the five-tone repeating unit would be represented in memory. The mismatch negativity component of event-related brain potentials was used to index how the sounds were organized in memory when participants had no task with the sounds. Only at the 200-ms onset-to-onset pace was the five-tone sequence unitized in memory. At presentation rates of 400 ms and above, the regularity (a different frequency tone occurred every fifth tone) was not detected and mismatch negativity was elicited by these tones in the sequence. The results show that temporal proximity plays a role in unitizing successive sounds in auditory memory. These results also suggest that global relationships between successive sounds are represented at the level of auditory cortices.

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Introduction

Unraveling the mysteries of human perception might be one of the most fascinating and difficult challenges in cognitive sciences. We usually have little regard for this, but at every single moment, we achieve something outstanding: By forming a coherent representation from the tangled mess of external stimuli that reach our sensory organs, we make sense of the outside world. In doing so and seemingly effortlessly, we overcome complicated mathematical and philosophical problems. Recent advances in emerging fields like computer vision and machine hearing have provided a sense of how daunting these tasks can be—requiring complex models that consume vast amounts of computational resources and energy. What enables the brain to fulfill these functions with such ease while consuming no more than the power equivalent of a lightbulb?

Over the centuries, many theories have been broad forward in an attempt to answer these questions. While early philosophers like Aristotle believed in the idea of direct or naïve realism (the idea that the outside world is perceived directly), early modern scholars like John Locke promoted the concept of indirect realism, which is highly compatible with the assumption of representationalism in cognitive science (perceptual experiences result from an internal representation rather than directly from external objects). Among the first who developed a consistent theory defining the rules followed by indirect perception were the Gestalt psychologists of the early 20th century. Wertheimer, Koffka, and Köhler hypothesized that Gestalt principles, self-organizing rules on how individual elements should be grouped or separated, guide perception. Intriguingly, they based their principle on the observation that humans perceive a global whole instead of just collections of individual parts.

Much later, auditory scientists faced the same challenges described in the first paragraph, but now in a very particular context: They were puzzled by the brain's ability to convert small air pressure fluctuations into actual auditory percepts. Somehow, the brain forms meaningful perceptual experiences from what can only be described as a busy mess of sound waves that originate from a plethora of different sources differing in pitch, loudness, and spatial position. Known as the *cocktail party effect* (Cherry, 1953), this problem was compared to inferring the

positions, shapes, and movements of motorboats on a lake—just by observing how two nearby objects move up and down the waves. Attempts to find answers to this perplexing question lead to the development of auditory scene analysis (ASA). Not unlike the concepts proposed by the Gestalt theorists six decades earlier, Bregman (1990) suggested that the brain uses so-called *streaming* and *segregation* to form auditory objects from rich spectro-temporal information. At its core, ASA relies on two different categories of grouping, namely *sequential* and *simultaneous* integration: Simultaneous integration (or vertical integration) refers to the grouping of concurrent properties into one or more separable auditory objects, a process informed by temporal cues like common onset and offset, spectral and spatial characteristics. Sequential integration (or horizontal integration), on the other hand, describes how temporally distinct sounds are merged into one or multiple coherently perceived streams (contrary to auditory objects in simultaneous grouping, only one such stream can be actively perceived at any time). While vertical and horizontal grouping can come to different and therefore competing results, sequential grouping often takes precedence over cues for simulations integration (Bendixen, 2014).

Often, the key to understanding such complex phenomena lies in learning about the most basic processing steps. In auditory research, these steps usually come in the shape of very simple stimuli, often consisting of nothing more than pure tones. Such stimuli were also the first to be used in the auditory oddball paradigm, a now well-established and robust paradigm extensively used in event-related potential (ERP) studies (Squires et al., 1975). In its basic form, participants are presented with a series of similar tones or sounds (so-called *standard* events), interrupted by rare tones or sounds that differ in at least one feature (*deviant* events) from the more frequent ones. Strikingly, deviant events elicit more extensive neural activity over sensory areas. This finding is known as the mismatch negativity (MMN) component because when measured using electroencephalography (EEG), a robust negative deflection can be observed in the difference wave obtained by subtracting the response to standard events from the response to deviant events. Negativity is strongest in the frontotemporal area of the scalp, with a peak latency ranging from 100 to 250 ms after stimulus onset. The MMN is not only elicited by individual rare deviant tones embedded in a stream of frequent tones but can also arise in the

presence of complex rule violations, i.e. when abstract auditory regularities are violated (Paavilainen, 2013). MMNs resulting from violations of regularities based on complex auditory regularities are referred to as *pattern MMN* from hereon. Complex auditory regularities can come, for example, in the form of the direction of frequency changes in tone pairs (e.g., Saarinen et al., 1992), infrequent shortenings of SOA (Ford & Hillyard, 1981), multiple tones (Alain et al., 1994; Schröger et al., 1996).

Interestingly, implications from MMN components are highly compatible with another prevalent theory of perception, namely the idea that perception is not a stimulus-driven bottom-up process but is informed by internal predictions. Despite their recent popularity, these ideas have been around for a long time and famously trace back to the physiologist Hermann von Helmholtz. Gregory's notion of "perception as hypotheses" is similarly well-known. Most recently, this notion has been introduced as a theory known as hierarchical predictive coding. Predictive coding specifically suggests that at every processing state, predictions from so-called *probabilistic generative models* and sensory input are compared continuously, and only their difference, termed *prediction error*, is propagated. MMN responses have been proposed as an index of prediction error (Wacongne et al., 2011). Although other interpretations exist (e.g., Bregman, 1990; May & Tiitinen, 2010), the MMN is frequently interpreted as a marker of expectation violations—a notion particularly emphasizing the role that predictions plays in perception (e.g., István Winkler, 2007).

An interesting situation arises when concurrent predictive clues exist. Following this idea, Sussman et al. (1998) presented participants with a sequence of frequent pure tones and rare pitch deviants while reading a book of their choice. Tones were arranged in a predictable five-tone pattern consisting of four standard tones and one deviant (i.e., A-A-A-B-A-A-A-B-A-A-A-B-A-A-A-B). "-" indicating silence between the tones). ERPs to A and B tones were compared for rapid (SOA of 100 ms) and slow (SOA of 1300 ms) stimulation rates. The 100 ms SOA presentation also included a control condition in which tone order was pseudo-random (e.g., A-A-A-B-A-B-A-A) but without altering deviant occurrence probability (Pr(B) = .20). When the presentation is random, only the relative occurrence frequency of tones carries value for

predicting the next tone. This, we refer to as *proportional regularity*. However, in an ordered presentation, a sequence of four standard tones is always followed by one deviant tone. Thus, understanding this relationship should allow for *perfect prediction* in which all deviant tones can be expected with near-absolute certainty. We call this regularity a *pattern regularity*. Provided the underlying mechanism can incorporate such information, the pitch deviants' processing should correspond to that of standard tones, and therefore no MMN should be elicited.

Interestingly, in Sussman et al., MMNs were only elicited if tone presentation was slow and predictable or fast and random, but not when predictable tones were presented rapidly. In a subsequent study, Sussman & Gumenyuk (2005) used the same pattern at different SOAs (200 ms, 400 ms, and 800 ms). Similar to their previous study, grouped presentation at 400 ms and 800 ms SOA elicited an MMN response, while at a stimulation rate of 200 ms, evidence for such a deflection was absent. Sussman et al. attributed this observation to sensory memory limitations. That is, only when auditory memory can accommodate enough repetitions of the five-tone pattern; can the brain integrate tones into a coherent representation allowing for accurate predictions of deviant tones. In turn, this would explain the absence of MMNs when the presentation was fast and ordered. Based on this, they argued that while valid for fast presentation rates with SOAs up to 200 ms, for longer SOAs, pattern durations would be too long, and thus representations would exceed sensory memory capacity.

In a recent in-class replication study, Scharf & Müller (in prep) presented participants with the same stimuli as Sussmann et al. in a very similar experimental setting. Their study only differed in that participants were assigned a simple task in which they had to count visual targets instead of reading a book of their choice. Surprisingly, while descriptive results were compatible with Sussmann et al., pairwise comparisons revealed no significant effect when comparing deviant and standard tones for both the *random* and the *predictable* condition. Further Bayesian analysis remained largely inconclusive, providing only *anecdotal* evidence in favor of the aforementioned effect for *random* presentation and *moderate* evidence for its absence in the *predictable* condition. In the face of the replication crisis, many scientists have become painfully aware of the importance of replicability (Ioannidis, 2005). Exact or quasi-exact replication

studies that try to match the original study's experimental conditions as closely as possible are regarded as the gold standard of science (Jasny et al., 2011; Popper, 1935). However, replications that extend, change, or optimize materials or methods of the original work also offer valuable insight. This kind of replication is known as conceptual (Schmidt, 2009) and refers to using different methods to repeat the test of a hypothesis or experimental result.

Hypothesis, Aims, and Objectives This thesis seeks to replicate Sussman et al.'s findings. It mainly follows the procure laid out by Sussman & Gumenyuk (2005). However, it deviates from the original design in some critical aspects. First, the aforementioned five-tone patterns are presented in both the *predictable* condition and in the *random* context. That is, pseudo-random order will be deliberately broken by occasionally presenting (B-)A-A-A-B-patterns. In particular, this will ensure that the local history of B-tones in the *random* condition is comparable to that in the *predictable* condition. Also, B tones are compared exclusively with their preceding A tones. Lastly, a small number of A-A-A-B will be replaced by A-A-A-A sequences in both conditions, allowing for the comparison of physically identical tones in different contexts. The advantage of this design is discussed in more detail in the following paragraphs. A pre-registration covering data collection, processing, and analysis is available at https://osf.io/cg2zd/. Deviations from this pre-specified plan and further exploratory analyses are explicitly reported.

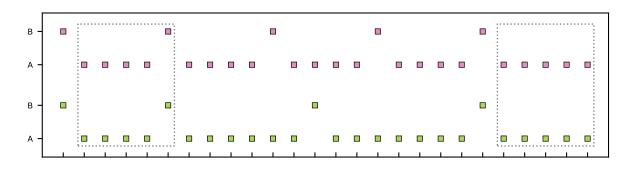
Sussman & Gumenyuk (2005) interpretation of the original results suggests that at fast stimulation rates (SOA of 200 ms and faster), extracted pattern-based regularities take precedence over proportion-based regularities. If this is true, B-tones in the *predictable* condition should not be considered a *mismatch* and should not elicit an MMN response. In contrast, since there is no way to predict B-tones in the *random* condition reliably, these tones would still be considered *deviant* events and are therefore expected to generate an MMN. On the other hand, when an A tone replaces a predictable B tone, one would expect an MMN despite physically identical tones. Specifically, hypotheses are formulated in regards to the ERPs elicited by the 5th tone in the five-tone sequence (A-A-A-A-B or A-A-A-A; boldface marks tone of interest) compared to the 4th tone in that sequence (A-A-A-A-X, "X" marking either an A or a B tone).

Suppose Sussman's interpretation holds, one expects negativity in the N1/MMN time range (about 100-200 ms after tone onset) for deviations in the B-A-A-A-B sequence in the random condition since B tones violate the $proportional\ regularity$ within the local context. This kind of response will hereinafter be referred to as a $local\ MMN$. Besides, one expects no evidence for such an effect (or evidence favoring \mathcal{H}_0 , i.e., that there is no effect) in the predictable context since more informative higher-order predictions based on $pattern\ regularity$ are not violated. Since MMNs should only be observed in one of the conditions, MMNs responses should differ between conditions. Lastly, the comparison between the 5th A tone and the proceeding A tone (A-A-A-A-X vs. A-A-A-A) should be considered a mismatch as the rare pattern (A-A-A-A) violates the more frequent pattern (A-A-A-B) and is therefore expected to elicit a significant pattern MMN response.

However, other results than those assumed by the original authors are conceivable. Here, two additional theoretical considerations that could explain divergent results will be discussed shortly. Of these, the first one is that the auditory system may not be able to extract complex patterns and therefore relies entirely on proportional regularities. In this case, no pattern regularity is extracted, and B-tones should result in a local MMN response regardless of presentation context since the predictive value of the proportional regularity does not vary between conditions. Furthermore, this notion implies that local MMN responses would not differ between conditions. Similarly, when violating the pattern regularity by introducing rare A tones at the fifth place of the predictable sequence, no pattern MMN should be triggered since A tones do not constitute a mismatch under this premise. As a second possibility, the brain might use proportional regularities and pattern regularities concurrently, resulting in a local MMN following B-tones in either condition. When violating the pattern regularity by presenting A tones at fifth place, these tones should be detected as deviants and therefore result in a pattern MMN.

Figure 1.

Caption



Method

Participants

All participants were recruited at the Institute of Psychology at the University of Leipzig and reported good general health, normal hearing, and normal or corrected-to-normal vision.

Written informed consent was obtained before the experiment. Participants were blinded to the purpose of the experiment and received compensation in course credit or money.

For the 100 ms presentation rate, data were collected from twenty participants (2 males, average age 22.3 yrs., SD=6.46, range 18 - 41 yrs.). The sample for the 150 ms presentation rate consisted of twenty-three psychology undergraduate students (2 males, average age 22.6 yrs., SD=5.57, range 18 - 42). Here, participants were also asked to provide information regarding their prior musical training: at the time of the survey, approximately one-third (34.8%) of participants engaged in musical activities, while 8.7% had no prior musical experience.

Procedure and Stimuli

Participants sat in a comfortable chair in a sound-insulated chamber. The experimental setup was practically identical to that of Sussman et al.; however, instead of reading a book, subjects were asked to direct their attention to a self-selected movie. Movies were presented with subtitles but without sound. Commercially available software (MATLAB R2014a; The MathWorks Inc, Natick, MA) in conjunction with the Psychophysics Toolbox extension (version 3.0.12, Brainard, 1997; Kleiner et al., 2007) was used to control stimulus presentation. Stimuli

consisted of pure sinusoidal tones with a duration of 50 ms (including a 10 ms cosine on/off ramp), presented isochronously at a stimulation onsets asynchrony (SOA) of 100 ms or 150 ms, respectively. Tone presentation was blocked and participants had the option to take a break after each block. Blocks contained 820 frequent 440 Hz tones ("A" tones) and 180 infrequent 449 Hz tones ("B" tones), delivered binaurally using Sennheiser HD-25-1 II headphones at 70 dB ($p_B = .18$, fixed for both conditions). For the 100 ms condition, participants were presented with 40 blocks, while 20 blocks were presented in the 150 ms condition. In one-half of the blocks, tones occurred in pseudo-random order (e.g., A-A-A-B-A-B-A), random condition) while in the other half, tone presentation followed a simple pattern in which a five-tone-sequence of four frequent tones and one infrequent tone (i.e., A-A-A-B) was repeated cyclically (predictable condition). Block order was counterbalanced across participants. Additionally, A tones replaced 10% of designated (infrequent) B tones in the predictable condition, resulting in sporadic five-tone sequences consisting solely of A tones (i.e., A-A-A-A), thus violating the pattern regularity. To assure comparability of local histories between tones of interest in both conditions, pseudo-randomly arranged tones were interspersed with sequences matching those from the predictable condition (i.e., B-A-A-A-A-B-A and B-A-A-A-A-A). Care was taken that sequences in the random condition were always sepearated by at least five pseudo-random tones and that in the predictable condition, A-A-A-A-patterns were always seperated by at least two A-A-A-B-patterns. A total of 20,000 tones at 150 ms SOA or 40,000 tones at 100 ms SOA were delivered to each participant resulting in a total duration (exluding potential breaks) of 1 hour and 7 minutes (100 ms SOA) and 50 minutes (150 ms SOA), respectively.

Tones of Interest. For all sequences, the finth B or A tones (A-A-A-B or A-A-A-A, boldface marks tone of interest) were compared to the peceding A tones (A-A-A-A-X). In For the 150 ms presentation rate, this setup resulted in 200 5th B tones, 200 5th A tones, and 400 4th A tones in the *random* condition; and 1800 5th B tones, 200 5th A tones and 2000 4th A tones in the *predictable* condition. For the 100 ms SOA, number of tones was doubled: 400 () 5th B tones, 400 () 5th A tones, and 800 () 4th A tones in the *random* condition; and 3600 () 5th B tones, 400 () 5th A tones and 4000 () 4th A tones in the *predictable* condition. Numbers in parenthesis indicate average number of epochs after preprocessing.

Data Acquisition

Electrophysiological data were recorded from active silver-silver-chloride (*Ag-AgCl*) electrodes using an ActiveTwo amplifier system (BioSemi B.V., Amsterdam, The Netherlands). A total of 39 channels were obtained using a 32-electrode-cap and seven external electrodes. Scalp electrode locations conformed to the international 10–20 system. Horizontal and vertical eye movement was obtained using two bipolar configurations with electrodes placed around the lateral canthi of the eyes as well as above and below the right eye. Additionally, three electrodes were placed on the tip of the nose and at the left and right mastoid sites. Data were sampled at 512 Hz and on-line low-pass filtered at 1000 Hz.

Analysis Pipeline

Data preprossessing was implemented using a custom pipeline based on the *MNE Python* software package (Gramfort, 2013) using *Python 3.7*. Computations were partly carried out on a cluster operated by the University Computation Center of the University of Leipzig. Code used in this thesis is publicly available at https://github.com/marcpabst/xmas-oddballmatch.

First, EEG data were subjected to the ZapLine procedure (de Cheveigné, 2020) to remove line noise contamination. A fivefold detection procedure, as described by Bigdely-Shamlo et al. (2015) was then used to detect and subsequently interpolate bad channels. Namely, this included detecting channels that contained prolonged segments with very small values (i.e., flat channels), the exclusion of channels based on robust standard deviation (deviation criterion), unusually pronounced high-frequency noise (noisiness criterion), and the removal of channels that were poorly predicted by nearby channels (correlation criterion and predictability criterion). Channels considered bad by one or more of these methods were removed and interpolated using spherical splines (Perrin et al., 1989). Electrode locations for interpolations were informed by the BESA Spherical Head Model.

For independent component analysis (ICA), a 1-Hz-high-pass filter (134th order hamming-windowed FIR) was applied (Irene Winkler et al., 2015). Artifact Subspace Reconstruction (ASR, Mullen et al., 2015) was used to identify and remove parts of the data with

unusual noise characteristics (bursts). ICA was then carried out using the *Picard* algorithm (Ablin et al., 2018, 2017) on principal-component-analysis—whitened (PCA) data. PCA was also used for dimensionality reduction to avoid rank-deficiency when extracting components from data with one or more interpolated channels. The EEGLAB (version 2020.0, Delorme & Makeig, 2004) software package and the IClabel plugin (version 1.2.6, Pion-Tonachini et al., 2019) were used to classify estimated components automatically. Only components clearly classified (i.e., confidence above 50%) resulting from either eye movement, muscular, or heartbeat activity were zeroed-out before applying the mixing matrix to unfiltered data [^1]. A-A-A-A-B, [^1]: The pre-registration states that ICA components should be reviewed by two experianced analysts. It should be noted that this procedure deviated from the pre-registration in that it was fully automated.

In line with recommendations from Widmann et al. (2015) and de Cheveigné & Nelken (2019), a finite impulse response (FIR) bandpass filter from 0.1 Hz to 40 Hz (Hamming window, 0.1 Hz lower bandwidth, 5 Hz upper bandwidth, 0.0194 passband ripple, and 53 dB stopband attenuation) was applied. Continuous data were epoched into 400 ms long segments around stimulus onsets, including a 100 ms pre-stimulus interval. No baseline correction was applied, and segments exceeding a peak-to-peak voltage difference of 100 μ V were removed. On average, (TODO) epochs were dopped. No dataset met the pre-registered exclusion criterion of less than 100 valid trials per condition; thus, data from all participants (20 for 100 ms presentation rate and 23 for 150 ms presentation rate) were included in the analysis.

Statistical Analysis

Statistical analysis was carried out using the *R* programming language (version 3.2, The R Core Team) using the *rstatix* package (version 2.0, Kassambara, 2020).

Mismatch Negativity. Calculation of the dependant variable followed the original study's procedure in averaging amplitudes in a time window extending ±25 ms around the expected peak of negativity. Specifically, this peak was obtained by subtracting the average ERP following the A tones from the average ERP following B tones in the *random condition* for both presentation rates separately. To compute mean amplitudes, ERPs to 4th position A tones

(A-A-A-A-X, **boldface** indicates the tone of interest) and B tones (A-A-A-B) were averaged separately for both the *random* and the *predictable condition*. For the *random condition*, only tones presented as part of a sequence matching the patterns from the *predictable* condition were included in the analysis. This set up resulted in

In accordance with the original analysis by Sussman & Gumenyuk (2005), mean amplitudes for frontocentral electrodes (pooled FZ, F3, F4, FC1, and FC2) and the two mastoid positions (pooled M1 and M2) were averaged separately. Then, for both SOAs, independent two-way repeated-measures analyses of variance (ANOVA) with factors *condition* (levels *predictable* and *random*), *stimulus type* (levels *A tone* and *B tone*), and their interaction were calculated. Following this, significant interaction effects were further investigated using post-hoc *t*-tests.

Bayesian Analysis. Going beyond the original study and extending the pre-registered procedure, Bayesian analysis was conducted for ANOVA posthoc comparisons. As mentioned above, traditional null hypothesis testing has some limitations that are often overlooked, leading to incorrect conclusions drawn from results. For example, not rejecting the null hypothesis ("non-significance") can usually not be interpreted as evidence in favor of the null hypothesis (e.g., Aczel et al., 2018; Goodman, 2008; Kirk, 1996; Meehl, 1978). Similarly, p-values might exaggerate evidence against \mathcal{H}_0 (that is, observed data might be more likely under \mathcal{H}_0 than under \mathcal{H}_1 even tough \mathcal{H}_0 is rejected, e.g., Hubbard & Lindsay, 2008; Rouder et al., 2009; Sellke et al., 2001; Wagenmakers et al., 2018). Conversely, Bayesian hypothesis testing using Bayes factors can provide an intuitive way to compare observed data's likelihood under the null hypothesis versus the alternative hypothesis (Wagenmakers, 2007), thereby making it possible to evaluate the null hypothesis: $BF_{10} = \frac{Pr(data|\mathcal{H}_0)}{Pr(data|\mathcal{H}_1)}$. Here, this approach was applied in agreement with the concept described by Rouder et al. (2009) as an alternative to classical frequentist paired t-tests. Following their sentiment, Bayes factors for within-participant differences γ_i were computed assuming $\mathcal{H}_0: y_i \sim Normal(0, \sigma^2)$ and $\mathcal{H}_1: y_i \sim Normal(\delta, \sigma^2); \delta \sim Cauchy(0, 1/\sqrt{2})$. A Jeffreys prior was used for the variance σ^2 in both models: $p(\sigma^2) \propto 1/\sigma^2$. Calculations were performed using the Hamiltonian Monte Carlo method implemented in Stan (version 2.25,

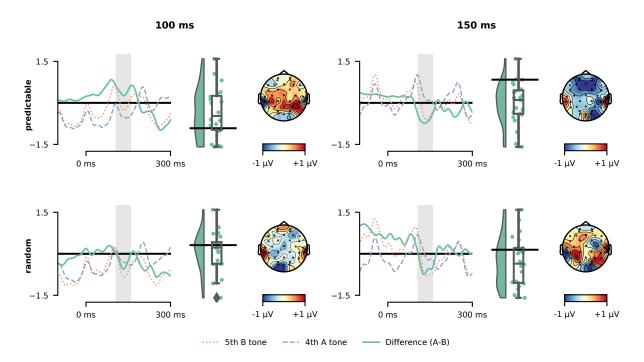
Carpenter et al., 2017) and RStan (Stan Development Team, 2020).

Reliability Analysis. Finally, the relationship between epoch number and the reliability of the estimate was analyzed by drawing random subsamples of different sizes from both data sets and calculating split-half reliability employing the Spearman–Brown approach. Thus, single-trial responses for all A and B tones in the predictable condition were randomly shuffled. Then, $100, 200, ..., N_{max}$ ($N_{max,100ms} = 2500, N_{max,150ms} = 1300$) epochs were drawn, randomly assigned to one of two halves, and averaged separately for A and B tones. Then, split-half reliability was calculated based on the mean amplitude in the MMN latency window as defined above. The Spearman–Brown prophecy formula¹ (Brown, 1910; Spearman, 1910) was used to obtain corrected reliability. This procedure was repeated 100 times for each N, and split-half-reliabilities obtained as such were subsequently averaged.

 $^{^1}$ as given by $\rho_{xx'}=\frac{2\rho_{12}}{1+\rho_{12}}$, where ρ_{12} is the Pearson correlation coefficient between the two halfes.

FIGURE 2.

ERP grand averages (pooled FZ, F3, F4, FC1, and FC2 electrode locations) for an SOA of 100 ms (left) and 150 ms (right), for A tones (A-A-A-A-X, blue dashed lines) and B tones (A-A-A-B, orange dashed line) and their difference (B - A, green solid line). Upper panels show ERPs for tones presented in a predcitable pattern (predcitable condition) while lower panels show ERPs for tones presented in pseudo-random order (random condition). Shaded area marks MMN latency window (110 ms to 160 ms) used to calculate the distribution of amplitude differences across participants (middle of each panel) and the difference of topographic maps averaged over the same interval (right of each panel).

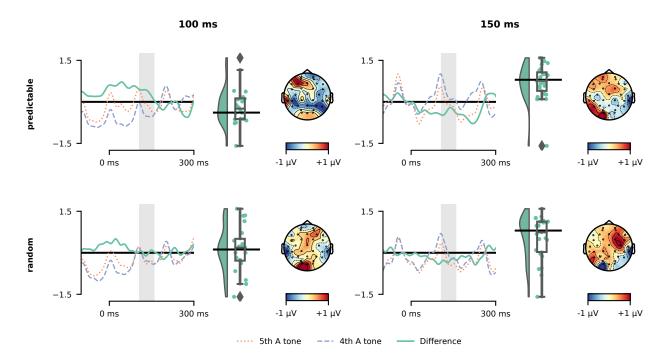


Results

Fig. 2 displays grand averages of event-related potentials (ERP) at pooled FZ, F3, F4, FC1, and FC2 electrode locations to A tones (A-A-A-A-X), B tones (A-A-A-B), and their difference (B tone minus A tone) for both 100 ms (left panel) and 150 ms (right panel) SOAs. The top half of each panel shows ERPs in the *predictable condition* while the lower half depicts ERPs in the *random condition*. Clearly visible rhythms result from fast presentation frequencies and illustrate the considerable overlap between neighboring tones. Panels also show the distribution of mean amplitude differences in the MMN latency window across participants and the difference of scalp topographies. Similarly, waveforms and mean amplitude difference distributions at pooled

FIGURE 3.

ERP grand averages (pooled FZ, F3, F4, FC1, and FC2 electrode locations) for an SOA of 100 ms (left) and 150 ms (right), for 4th A tones (A-A-A-A-X, blue dashed lines) and 5th A tones (A-A-A-A, orange dashed line) and their difference (B - A, green solid line). Upper panels show ERPs for tones presented in a predcitable pattern (predcitable condition) while lower panels show ERPs for tones presented in pseudo-random order (random condition). Shaded area marks MMN latency window (110 ms to 160 ms) used to calculate the distribution of amplitude differences across participants (middle of each panel) and the difference of topographic maps averaged over the same interval (right of each panel).



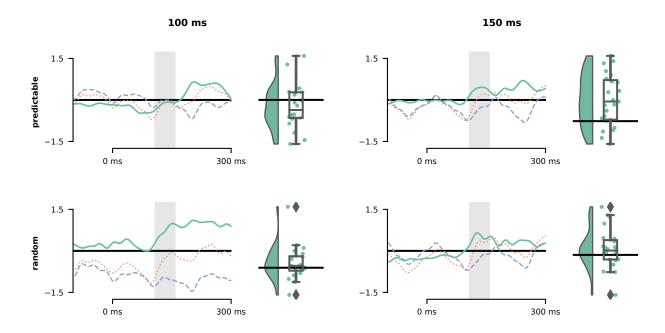
mastoid sites are shown in fig. 4.

100 ms Presentation Rate. The MMN latency window was determined to range from 108 ms to 158 ms ofter stimilus onset. Descriptively, mean amplitudes at pooled frontocentral electrode locations were more negative for randomly presented B tones than for randomly presented A tones ($\Delta M = -0.361~\mu V$). Strikingly however, B tones seemed to elicit more positive responses than associated A tones ($\Delta M = 0.379~\mu V$).

ANOVA results for the frontocentral electrode cluster revealed a significant effect of the interaction term (condition x stimulus type; F(1, 19) = 17.00, p = 0.0006) indicating that difference waves for A and B tones differed between condition. Complementary analysis for 4th

FIGURE 4.

ERP grand averages (pooled M1, M2 electrode locations) for an SOA of 100 ms (left) and 150 ms (right), for A tones (A-A-A-A-X, blue dashed lines) and B tones (A-A-A-B, orange dashed line) and their difference (B - A, green solid line). Upper panels show ERPs for tones presented in a predcitable pattern (predcitable condition) while lower panels show ERPs for tones presented in pseudo-random order (random condition). Shaded area marks MMN latency window (110 ms to 160 ms) used to calculate the distribution of amplitude differences across participants.



A tones and the 5th A tones (A-A-A-A-X versus A-A-A-A; Table 2) did not result in any significant effects.

Two-tailed Student's t-tests and complementary Bayesian analysis were used to test MMN responses at the frontocentral electrode cluster for significance from zero. The Benjamini–Hochberg step-up procedure was employed to correct p-values for multiple comparisons. Results indicated that B tones eclicted more positive responses compared to A tones when presented in a predictable context (t(19) = -2.81, p = .022, $CI_{.95} = [-0.66, -0.10], BF_{10} = 4.65$). Although descriptive statistics suggested a contrary effect for randomly presented tones, results remained inconclusive (t(19) = 1.69, p = .173, $CI_{.95} = [-0.09, 0.81], BF_{10} = 0.77$).

Table 1.

Results of the 2-way ANOVA (condition x stimulus type) for repeated measures. Only fronto included.

		Effect	DFn	DFd	F	p	p<.05	ges
100 ms	Frontal	Condition	1	19	0.026	.873		0.000441
		StimulusType	1	19	0.938	.345		0.002
		Condition x StimulusType	1	19	0.961	.339		0.002
	Mastoids	Condition	1	19	3.59	.073		0.063
		StimulusType	1	19	1	.330		0.003
		Condition x StimulusType	1	19	0.822	.376		0.005
150 ms	Frontal	Condition	1	22	0.938	.343		0.003
		StimulusType	1	22	1.6	.219		0.008
		Condition x StimulusType	1	22	0.074	.789		0.000258
	Mastoids	Condition	1	22	0.875	.360		0.005
		StimulusType	1	22	2.8	.109		0.009
		Condition x StimulusType	1	22	0.93	.345		0.003

150 ms Presentation Rate. Calculation of MMN window of interest resulted in an interval from 104 ms to 154 ms after stimulus onset. Descriptivly, B tones in that interval were more negative than corresponding A tones for both predcitable ($\Delta M = -0.588 \ \mu V$) and random condition ($\Delta M = -0.518 \ \mu V$). ANOVA results suggested a main effect of factor stimulus type for both frontocentral (F(1,22)=21.62, p<.001) and mastoid electrodes (F(1,22)=6.26, p=0.0200). Since no significant interaction effect was present, no follow-up tests were performed.

Analysing Split-Half-Reliabilities. Average split-half reliabilities (Fig. 6) demonstrate that reliability can be characterized as a function of epoch number. Whereas a high number of epochs provided reasonable reliability, particularly small samples resulted in highly unreliable estimates. This observation might serve as a plausible explanation for the inconclusive result in the 100 ms

FIGURE 5.

Averaged voltages in the MMN latency window for pooled frontocentral and mastoid electrodes. Colored areas show sample probability density function for A tones (green) and B tones (red). White diamonds indicate estimated population mean, vertical bars represent 95%-conficence interval.

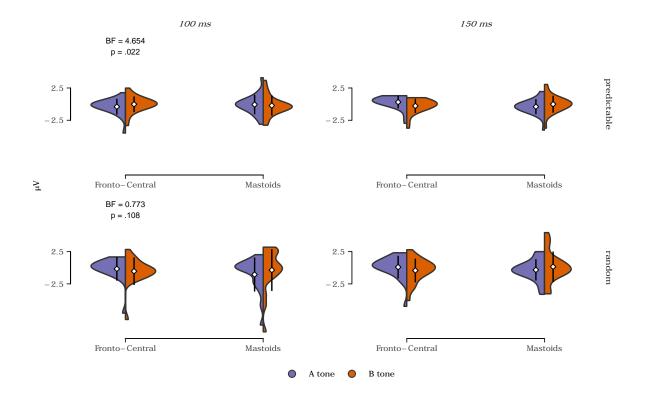


FIGURE 6.

Average split-half reliabilities for A and B tones in random and predictable contexts.. Negative values might be interpreted as low or no reliability (Cronbach & Hartmann, 1954). Thin lines in the 150 ms condition indicate extrapolation using the Spearman-Brown formula.

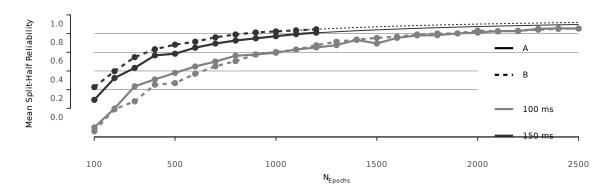


TABLE 2.

Results of the 2-way ANOVA (condition x stimulus type) for repeated measures. Only fronto included.

		Effect	DFn	DFd	F	p	p<.05	ges
100 ms	Frontal	Condition	1	19	0.137	.715		0.002
		StimulusType	1	19	0.004	.953		8.21e-06
		Condition x StimulusType	1	19	17	< .001	*	0.013
	Mastoids	Condition	1	19	1.39	.253		0.015
		StimulusType	1	19	0.946	.343		0.003
		Condition x StimulusType	1	19	2.2	.154		0.008
150 ms	Frontal	Condition	1	22	0.775	.388		0.005
		StimulusType	1	22	21.6	< .001	*	0.036
		Condition x StimulusType	1	22	0.194	.664		0.000147
	Mastoids	Condition	1	22	0.187	.670		0.001
		StimulusType	1	22	6.26	.020	*	0.017
		Condition x StimulusType	1	22	0.102	.753		0.000236

condition, as epoch numbers for B tones ($N_{avg}=364.4$) could be inadequately low to obtain a reliable estimate. In comparison, including all B tones (instead of only tones that were part of a five-tone pattern and akin to Sussman & Gumenyuk (2005)), on average led to an eightfold increase in epoch numbers ($N_{avg}=2919.8$). Interestingly, statistical comparison for such an extended sample was no longer inconclusive but indicated strong evidence in favor of more negative responses to B tones than to A tones (t(19)=3.31, p=.004, $CI_{.95}=[0.20,0.88], BF_{10}=11.92$).

Discussion

When presenting rare deviant tones in a stream of frequent standard tones, deviant tones elicit more negative EEG potentials than standard tones. Known as the mismatch negativity (MMN), this finding is one of the most well-studied phenomena in auditory neuroscience. This thesis aimed to conceptually replicate findings reported by earlier studies that suggested that no MMN is generated if certain contextual information is available. Specifically, Sussman et al. (1998) and Sussman & Gumenyuk (2005) proposed that recurring tone sequences at fast SOAs would be processed as a single auditory object. That is, sequences of tones presented in close temporal proximity should be sequentially grouped, and both standard and deviant tones would be fully integrated into this representation. Thus, deviant tones presented as part of these sequences should not constitute a *mismatch* since tones may be predictable as part of the sequence. Indeed, the original authors found no MMN response for deviants that were predictable in that they were presented as part of a recurrent pattern (*predictable condition*) and presented at SOAs of 200 ms or faster. Conversely, a clear MMN response was elicited by deviants when presentation followed no regular patter (*random condition*) or presentation rate was slower.

This thesis extends Sussman et al.'s work by introducing the five-tone sequences (A-A-A-A-B) from the *predictable* condition—consisting of four standard tones ("A") and one pitch deviant ("B")—into the *random* condition, allowing for comparisons between both conditions unaffected by differences in local pre-stimulus history. This, however, also meant that only a subset of all presented deviant tones were analyzes in the *random* condition. The original authors' interpretation suggested that B tones presented as part of the recurrent pattern should not be processed as deviants and therefore no MMN should be elicited in the *predictable condition*. The *random* condition served as a control in which one would expect strong evidence for an MMN response following classical oddbal litarture. Going boyond Sussman et al., it was also hypothized that tone because five-tone sequences would form a single auditory object, rare pattern violations created by replacing the deviant tone with a standard tone (i.e., A-A-A) would elicit an MMN response altough consiting of five physically identical tones. Indexing

TABLE 3.

This tables gives an overview of the statistical hypotheses tested and the expected outcomes (upper half). The lower half shoes results from the 100 ms SOA condition and the 150 ms SOA condition.

	Predictab	Difference Wave				
	$\mathcal{H}_1: B_{5th} < A_{4th}$	$\mathcal{H}_1: A_{5th} < A_{4th}$	$\mathcal{H}_1: \Lambda_{\mathit{rand}} \neq \Lambda_{\mathit{pred}}$			
Expected Pattern Secondary Hypotheses						
Only pattern regularities used	×	\checkmark	\checkmark			
Only Proportional regularities used	\checkmark	×	×			
Concurrent usage	\checkmark	\checkmark				
Results						
100 ms SOA	×*	n.s.	\checkmark			
150 ms SOA	✓	n.s.	n.s.			

 $[\]checkmark \colon \mathcal{H}_1 \text{ is true} \ / \ \mathcal{H}_0 \text{ rejected,} \times \colon \mathcal{H}_0 \text{ is true, } \textit{inc} \colon \text{inconclusive results} \sim \colon \text{no explicit expectation}$

violations of a more complex rule, this response was termed *pattern MMN* as opposed to *local MMN* elicited in response to local single-tone violations of proportional regularity.

Summary and Interpretation of Results

Several hypohtesis were considered in this thesis. Specifically, local MMN were investigated for the random and predicitable presentation. elictation local MMNs should be based on the extration and usage of *proportional regularity*, i.e., that standard tones are more frequent than deviant tones. Based on the account from Sussman et al. (1998) and Sussman & Gumenyuk (2005), local MMN should, however, not emerge when more informative *pattern regularirites* were present, assuming the underlyinogn neuronal machnims can extract and use these more complex rules. Table X gives an overview over the statistical hypotheses tested.

Local MMN in the Random Context. Deviant tones were expected to elicit more negative responses in the MMN latency range than standard tones when presented pseudo-randomly, as this condition mirrors the classical and well-proven auditory oddball paradigm. While this

hypothesis held for the slower presentation rate at an SOA of 150 ms, surprisingly, results for faster presentation (100 ms SOA) remained inconclusive when analyzing the originally defined subset of tones (3XX epochs on average). Simulating reliability for different sample sizes by subsampling from all deviants their directly preceding standard tone in the *random* condition revealed that epoch numbers used here might only offered low to moderate reliability. It is important to note, however, that power cannot be directly inferred from reliability, as realibility is inherantly a population-based measure (Humphreys & Drasgow, 1989). Nevertheless, increasing realibility (i.e, avoiding error of measurement) is an important aspect when increasing power (Zimmerman & Zumbo, 2015). Thus, this observation may be interpreted as an indication of low power, potentially explaining the absence of a significant effect. Interestingly, when the sample was expanded to include all deviant tones (4XXX epochs on average) - increasing the sample size at the cost of comparability with the *predictable* condition - strong evidence for an MMN was found. Taken together, small effect sizes, low reliability, and the fact that an MMN was found when including more deviant tone raise the question of whether power may have been simply too low to find a conclusive effect.

Local MMN in the Predictable Context. It was hypothesized that if the same tones are presented as part of a repeated five-tone sequence with no change in appearance probability, deviations should *not* elicit mismatch responses. While results remained inconclusive for faster presentation (100 ms SOA), contradictory evidence was found for data collected with an SOA of 150 ms. At the surface, results appeared to be inconsistent with the outcomes and conclusions from Sussman & Gumenyuk (2005), as a clear MMN was elicited in thr predictable condition. On closer inspection, however, it must be noted that Sussman & Gumenyuk (2005) interpreted the failure to find an effect as the absence of an effect. Therefore, results presented for the 150 ms SOA do not contradict the original findings but merely conflict with the authors' interpretation.

kkkk

Moreover, although seemingly at odds with Sussman's account, the results parallel those of more recent EEG and MEG studies. For instance, Bekinschtein et al. (2009) and Wacongne et al. (2011) found MMN responses for spectral deviants when presenting five-tone patterns

similar to those used in this thesis at an SOA of 150 ms. Analogous results using pure tones magnetoencephalography were obtained by Recasens et al. (2014) with an SOA of 200 ms.

Surprisingly, in the 100 ms condition, responses to predictable deviants were more positive in the MMN latency range than responses to standard tones. Challenging one's expectations and contradicting the results from the 150 ms condition, this observation was unexpected. However, visual inspection of the ERP trace revealed a possible explanation for this finding: pre-stimulus intervals exhibited apparent baseline differences that could have obscured real differences (or no differences) in responses. Thus, this result might have to be considered as an artifact of rapid stimulation. Possible approaches that remedy this problem and may be used to disentangle evoked responses from subsequent tones will be discussed in a later paragraph.

Contrasting local MNNs between Conditions. Based on the notion that local MMNs should only be eclicited in the random and not in the predcitable condition, local MMNs should differ between the two conditions. Statistical analysis provided support for this assumption only at the faster 100 ms presentation rate. However, this seems mainly to be driven by the more positive response to deviant tones in the predictable condition, as outlined above. Thus, this might not be taken as unconditional evidence in favor of aforementioned hypothesis and care must be taken when interpreting this effect.

Pattern-MMN. No conclusive results were found regarding the hypothesis that violations of the regular five-tone pattern would trigger an MMN response. This assumption was based on the notion of higher-order MMNs that should be elicited when violating patterns of multiple tones that are represented as a single auditory object. [...] There are several avenues to explain the lack of a detectable effect. First, epoch numbers [numbers, rel] were relatively small, and therefore statistical power may have been very low. Secondly, mechanisms underlying MMNs for simple local deviations might be different from those responsible for higher-order rule violations. An interesting line of research has suggested that pattern MMNs may involve different latencies than those explored in this study. For example, Bekinschtein et al. (2009) found that pattern deviations did not trigger MMNs at 150 ms SOA, but eclicited deflection at

later latencies (>300 ms after stimulus onset). Recasens et al. (2014) found no evidence for differences at erally latencies found that late MMNm responses (approximately 160 ms after stimulus onset) indexed pattern violations. Based on source reconstruction, authors also argued that neuronal generators engaged in the encoding of proportional regularities might be distinct from those encoding pattern regularities.

This notion is consistent with computer simulations suggesting that the cortical mechanisms underlying the processing of sensory information as indexed by the MMN response may operate at several different hierarchical levels, spanning from the level of simple stimuli to more complex patterns (Kiebel et al., 2008). There is growing support for this theoretical notion of hierarchical predictive coding in the auditory domain from empirical work (e.g., Cornella et al., 2012). When following this line of reasoning, detection of simple feature deviations should occur at lower cortical levels and therefore become apparent relatively early (i.e., within typical MMN latencies or earlier), whereas deviations from complex rules should be detected at higher cortical levels. Thus, effects in ERP would only become visible in later latencies.

In general, these findings might be better explained by a more general predictive coding framework than by the relatively narrow auditory integration-based account originally proposed by Sussman et al.. However, it remains unclear what role the SOA would play in this regard—it is still very much conceivable that short SOAs facilitate pattern extraction compared to slower stimuli presentation. Also, if knowledge of complex regularities is constituted at higher cortical levels, backpropagation might be used to inform mismatch detection at lower levels. While this, evidently, does not seem to result in a full suppression of MMNs to simple deviant tones, MMN responses might be partially diminished, thus explaining results from Sussman & Gumenyuk (2005).

Limitations and Future Research

In sum, results in the 150 ms condition contradict the interpretation of Sussman et al.. An MMN response was found regardless of whether deviant tones occurrend pseudo-randomly or in a predictable fashion, challenging the idea of a fully integrated representation of the five-tone

sequences. However, data collected with tones presented at an SOA of 100 ms remained inconclusive to a large extent due to two main problems. One the one hand, low epoch numbers reduce the reliability of results. On the other hand, the fast presentation rate made it challenging to interpret responses to subsequent tones due to considerable overlap between ERPs. Several approaches to disentangle individual responses have been suggested (e.g., Plourde et al., 1988; Woldorff, 1993). These options, however, often require specific stimulation patterns that predefine experimental designs. More recently proposed methods include regressions ERPs (Smith & Kutas, 2015; e.g., Ehinger & Dimigen, 2019), that allow separating responses to different stimuli employing multiple regression models. Due to collinearity, however, they tend to work poorly on stimuli presented with a constant SOA. One method to deal with this is to add jitter to stimulus onsets, although it remains unclear if jittered presentation would still lead to the proposed grouping of tone patterns in the paradigm used in this thesis.

It should also be noted that the original authors' filter parameters differed from those used in this thesis. In addition, the original study did not use ICA for artifact removal. However, it remains questionable whether this can fully account for the discrepancies found. Still, one might examine the impact of different preprocessing steps such as ICA, and baselining to improve the interpretability of results.. Recently introduced approaches such as multiverse analyses (Steegen et al., 2016) could provide additional transparency in reporting.

Conclusion

In conclusion, results from Sussman et al. (1998) were partially replicated while statistical analysis conflicting with the original authors' interpretation. Evidence was found for mismatch detection to simple proportional regularity violation even in the presence of a higher-order pattern. No pattern MMN was found at the lantencies used by Sussman et al. (1998). However, several statistical tests remained inconclusive or hard to interpret, probably due to low reliability and ERPs overlap from subsequent tones. Higher sample sizes and more sophisticated analysis methods might offer more insight but may need modification to the presentation procedure. [better ending]

References

- Ablin, P., Cardoso, J.-F., & Gramfort, A. (2018). Faster independent component analysis by preconditioning with Hessian approximations. *IEEE Transactions on Signal Processing*, 66(15), 4040–4049. https://doi.org/10.1109/TSP.2018.2844203
- Ablin, P., Cardoso, J.-F., & Gramfort, A. (2017). Faster ICA under orthogonal constraint. arXiv:1711.10873 [Stat]. http://arxiv.org/abs/1711.10873
- Aczel, B., Palfi, B., Szollosi, A., Kovacs, M., Szaszi, B., Szecsi, P., Zrubka, M., Gronau, Q. F., Bergh,
 D. van den, & Wagenmakers, E.-J. (2018). Quantifying Support for the Null Hypothesis in
 Psychology: An Empirical Investigation: Advances in Methods and Practices in Psychological
 Science. https://doi.org/10.1177/2515245918773742
- Alain, C., Woods, D. L., & Ogawa, K. H. (1994). Brain indices of automatic pattern processing: *NeuroReport*, 6(1), 140–144. https://doi.org/10.1097/00001756-199412300-00036
- Bekinschtein, T. A., Dehaene, S., Rohaut, B., Tadel, F., Cohen, L., & Naccache, L. (2009). Neural signature of the conscious processing of auditory regularities. *Proceedings of the National Academy of Sciences of the United States of America*, 106(5), 1672–1677. https://doi.org/10.1073/pnas.0809667106
- Bendixen, A. (2014). Predictability effects in auditory scene analysis: a review. *Frontiers in Neuroscience*, 8. https://doi.org/10.3389/fnins.2014.00060
- Bigdely-Shamlo, N., Mullen, T., Kothe, C., Su, K.-M., & Robbins, K. A. (2015). The PREP pipeline: standardized preprocessing for large-scale EEG analysis. *Frontiers in Neuroinformatics*, *9*. https://doi.org/10.3389/fninf.2015.00016
- Brainard, D. H. (1997). The Psychophysics Toolbox. *Spatial Vision*, *10*(4), 433–436. https://doi.org/10.1163/156856897X00357
- Bregman, A. (1990). Auditory scene analysis: the perceptual organization of sound. MIT Press.

Brown, W. (1910). SOME EXPERIMENTAL RESULTS IN THE CORRELATION OF MENTAL ABILITIES1. *British Journal of Psychology, 1904-1920, 3*(3), 296–322. https://doi.org/10.1111/j.2044-8295.1910.tb00207.x

- Carpenter, B., Gelman, A., Hoffman, M. D., Lee, D., Goodrich, B., Betancourt, M., Brubaker, M., Guo, J., Li, P., & Riddell, A. (2017). Stan: A Probabilistic Programming Language. *Journal of Statistical Software*, 76(1), 1–32. https://doi.org/10.18637/jss.v076.i01
- Cherry, E. C. (1953). Some Experiments on the Recognition of Speech, with One and with Two Ears. *The Journal of the Acoustical Society of America*, *25*(5), 975–979. https://doi.org/10.1121/1.1907229
- Cornella, M., Leung, S., Grimm, S., & Escera, C. (2012). Detection of Simple and Pattern Regularity Violations Occurs at Different Levels of the Auditory Hierarchy. *PLOS ONE*, *7*(8), e43604. https://doi.org/10.1371/journal.pone.0043604
- Cronbach, L. J., & Hartmann, W. (1954). A Note On Negative Reliabilities: *Educational and Psychological Measurement*. https://doi.org/10.1177/001316445401400213
- de Cheveigné, A. (2020). ZapLine: A simple and effective method to remove power line artifacts. *NeuroImage*, 207, 116356. https://doi.org/10.1016/j.neuroimage.2019.116356
- de Cheveigné, A., & Nelken, I. (2019). Filters: When, Why, and How (Not) to Use Them. *Neuron*, *102*(2), 280–293. https://doi.org/10.1016/j.neuron.2019.02.039
- Delorme, A., & Makeig, S. (2004). EEGLAB: an open source toolbox for analysis of single-trial EEG dynamics including independent component analysis. *Journal of Neuroscience Methods*, 134(1), 9–21. https://doi.org/10.1016/j.jneumeth.2003.10.009
- Ehinger, B. V., & Dimigen, O. (2019). Unfold: an integrated toolbox for overlap correction, non-linear modeling, and regression-based EEG analysis. *PeerJ*, *7*, e7838. https://doi.org/10.7717/peerj.7838

Ford, J. M., & Hillyard, S. A. (1981). Event-Related Potentials (ERPs) to Interruptions of a Steady Rhythm. *Psychophysiology*, *18*(3), 322–330. https://doi.org/https://doi.org/10.1111/j.1469-8986.1981.tb03043.x

- Goodman, S. (2008). A Dirty Dozen: Twelve P-Value Misconceptions. *Seminars in Hematology*, 45(3), 135–140. https://doi.org/10.1053/j.seminhematol.2008.04.003
- Gramfort, A. (2013). MEG and EEG data analysis with MNE-Python. *Frontiers in Neuroscience*, 7. https://doi.org/10.3389/fnins.2013.00267
- Hubbard, R., & Lindsay, R. M. (2008). Why P Values Are Not a Useful Measure of Evidence in Statistical Significance Testing: *Theory & Psychology*. https://doi.org/10.1177/0959354307086923
- Humphreys, L. G., & Drasgow, F. (1989). Some Comments on the Relation Between Reliability and Statistical Power. *Applied Psychological Measurement*, *13*(4), 419–425. https://doi.org/10.1177/014662168901300407
- Ioannidis, J. P. A. (2005). Why Most Published Research Findings Are False. *PLOS Medicine*, *2*(8), e124. https://doi.org/10.1371/journal.pmed.0020124
- Jasny, B. R., Chin, G., Chong, L., & Vignieri, S. (2011). Again, and Again, and Again *Science*, *334*(6060), 1225–1225. https://doi.org/10.1126/science.334.6060.1225
- Kassambara, A. (2020). rstatix: Pipe-friendly framework for basic statistical tests [Manual]. https://CRAN.R-project.org/package=rstatix
- Kiebel, S. J., Daunizeau, J., & Friston, K. J. (2008). A Hierarchy of Time-Scales and the Brain. PLOS Computational Biology, 4(11), e1000209. https://doi.org/10.1371/journal.pcbi.1000209
- Kirk, R. E. (1996). Practical Significance: A Concept Whose Time Has Come. *Educational and Psychological Measurement*, *56*(5), 746–759. https://doi.org/10.1177/0013164496056005002

Kleiner, M., Brainard, D., Pelli, D., Ingling, A., Murray, R., & Broussard, C. (2007). What's new in psychtoolbox-3. *Perception*, *36*(14), 1–16. https://nyuscholars.nyu.edu/en/publications/whats-new-in-psychtoolbox-3

- May, P. J. C., & Tiitinen, H. (2010). Mismatch negativity (MMN), the deviance-elicited auditory deflection, explained. *Psychophysiology*, *47*(1), 66–122. https://doi.org/https://doi.org/10.1111/j.1469-8986.2009.00856.x
- Meehl, P. E. (1978). Theoretical risks and tabular asterisks: Sir Karl, Sir Ronald, and the slow progress of soft psychology. *Journal of Consulting and Clinical Psychology*, *46*(4), 806–834. https://doi.org/10.1037/0022-006X.46.4.806
- Mullen, T. R., Kothe, C. A. E., Chi, Y. M., Ojeda, A., Kerth, T., Makeig, S., Jung, T.-P., & Cauwenberghs, G. (2015). Real-time neuroimaging and cognitive monitoring using wearable dry EEG. *IEEE Transactions on Biomedical Engineering*, *62*(11), 2553–2567. https://doi.org/10.1109/TBME.2015.2481482
- Paavilainen, P. (2013). The mismatch-negativity (MMN) component of the auditory event-related potential to violations of abstract regularities: A review. *International Journal of Psychophysiology*, 88(2), 109–123. https://doi.org/10.1016/j.ijpsycho.2013.03.015
- Perrin, F., Pernier, J., Bertrand, O., & Echallier, J. F. (1989). Spherical splines for scalp potential and current density mapping. *Electroencephalography and Clinical Neurophysiology*, *72*(2), 184–187. https://doi.org/10.1016/0013-4694(89)90180-6
- Pion-Tonachini, L., Kreutz-Delgado, K., & Makeig, S. (2019). ICLabel: An automated electroencephalographic independent component classifier, dataset, and website. *NeuroImage*, 198, 181–197. https://doi.org/10.1016/j.neuroimage.2019.05.026
- Plourde, G., Picton, T., & Kellett, A. (1988). Interweaving and overlapping of evoked potentials.

 Electroencephalography and Clinical Neurophysiology/Evoked Potentials Section, 71(6), 405–414.

 https://doi.org/10.1016/0168-5597(88)90044-5

Popper, K. (1935). Logik der Forschung: Zur Erkenntnistheorie der Modernen Naturwissenschaft. Springer Vienna.

- Recasens, M., Grimm, S., Wollbrink, A., Pantev, C., & Escera, C. (2014). Encoding of nested levels of acoustic regularity in hierarchically organized areas of the human auditory cortex. *Human Brain Mapping*, *35*(11), 5701–5716. https://doi.org/10.1002/hbm.22582
- Rouder, J. N., Speckman, P. L., Sun, D., Morey, R. D., & Iverson, G. (2009). Bayesian t tests for accepting and rejecting the null hypothesis. *Psychonomic Bulletin & Review*, 16(2), 225–237. https://doi.org/10.3758/PBR.16.2.225
- Saarinen, J., Paavilainen, P., Schöger, E., Tervaniemi, M., & Näätänen, R. (1992). Representation of abstract attributes of auditory stimuli in the human brain: *NeuroReport*, *3*(12), 1149–1151. https://doi.org/10.1097/00001756-199212000-00030
- Scharf, F., & Müller, D. (in prep). Predictable changes within fast-paced sound sequences do not elicit the mismatch negativity: An in-class replication study.
- Schmidt, S. (2009). Shall we Really do it Again? The Powerful Concept of Replication is Neglected in the Social Sciences: *Review of General Psychology*. https://doi.org/10.1037/a0015108
- Schröger, E., Tervaniemi, M., Wolff, C., & Näätänen, R. N. (1996). Preattentive periodicity detection in auditory patterns as governed by time and intensity information. *Cognitive Brain Research*, *4*(2), 145–148. https://doi.org/10.1016/0926-6410(96)00023-7
- Sellke, T., Bayarri, M. J., & Berger, J. O. (2001). Calibration of ρ Values for Testing Precise Null Hypotheses. *The American Statistician*, *55*(1), 62–71. https://doi.org/10.1198/000313001300339950
- Smith, N. J., & Kutas, M. (2015). Regression-based estimation of ERP waveforms: II. Nonlinear effects, overlap correction, and practical considerations. *Psychophysiology*, *52*(2), 169–181. https://doi.org/10.1111/psyp.12320

Spearman, C. (1910). Correlation calculated from faulty data. *British Journal of Psychology*, *3*, 271–295.

- Squires, N. K., Squires, K. C., & Hillyard, S. A. (1975). Two varieties of long-latency positive waves evoked by unpredictable auditory stimuli in man. *Electroencephalography and Clinical Neurophysiology*, *38*(4), 387–401. https://doi.org/10.1016/0013-4694(75)90263-1
- Stan Development Team. (2020). RStan: the R interface to Stan. http://mc-stan.org/
- Steegen, S., Tuerlinckx, F., Gelman, A., & Vanpaemel, W. (2016). Increasing Transparency
 Through a Multiverse Analysis. *Perspectives on Psychological Science: A Journal of the Association for Psychological Science*, 11(5), 702–712.

 https://doi.org/10.1177/1745691616658637
- Sussman, E. S., & Gumenyuk, V. (2005). Organization of sequential sounds in auditory memory: *NeuroReport*, *16*(13), 1519–1523. https://doi.org/10.1097/01.wnr.0000177002.35193.4c
- Sussman, E. S., Ritter, W., & Vaughan, H. G. (1998). Predictability of stimulus deviance and the mismatch negativity: *NeuroReport*, *9*(18), 4167–4170. https://doi.org/10.1097/00001756-199812210-00031
- Wacongne, C., Labyt, E., van Wassenhove, V., Bekinschtein, T., Naccache, L., & Dehaene, S. (2011).
 Evidence for a hierarchy of predictions and prediction errors in human cortex. *Proceedings of the National Academy of Sciences of the United States of America*, 108(51), 20754–20759.
 https://doi.org/10.1073/pnas.1117807108
- Wagenmakers, E.-J. (2007). A practical solution to the pervasive problems of pvalues.

 *Psychonomic Bulletin & Review, 14(5), 779–804. https://doi.org/10.3758/BF03194105
- Wagenmakers, E.-J., Marsman, M., Jamil, T., Ly, A., Verhagen, J., Love, J., Selker, R., Gronau, Q. F., Šmíra, M., Epskamp, S., Matzke, D., Rouder, J. N., & Morey, R. D. (2018). Bayesian inference for psychology. Part I: Theoretical advantages and practical ramifications. *Psychonomic Bulletin & Review*, 25(1), 35–57. https://doi.org/10.3758/s13423-017-1343-3

Widmann, A., Schröger, E., & Maess, B. (2015). Digital filter design for electrophysiological data – a practical approach. *Journal of Neuroscience Methods*, *250*, 34–46. https://doi.org/10.1016/j.jneumeth.2014.08.002

- Winkler, István. (2007). Interpreting the Mismatch Negativity. *Journal of Psychophysiology*, *21*(3-4), 147–163. https://doi.org/10.1027/0269-8803.21.34.147
- Winkler, Irene, Debener, S., Müller, K.-R., & Tangermann, M. (2015). On the influence of high-pass filtering on ICA-based artifact reduction in EEG-ERP. 2015 37th Annual International Conference of the IEEE Engineering in Medicine and Biology Society (EMBC), 4101–4105. https://doi.org/10.1109/EMBC.2015.7319296
- Woldorff, M. G. (1993). Distortion of ERP averages due to overlap from temporally adjacent ERPs: Analysis and correction. *Psychophysiology*, *30*(1), 98–119. https://doi.org/https://doi.org/10.1111/j.1469-8986.1993.tb03209.x
- Zimmerman, D., & Zumbo, B. (2015). Resolving the Issue of How Reliability is Related to Statistical Power: Adhering to Mathematical Definitions. *Journal of Modern Applied Statistical Methods*, *14*(2). https://doi.org/10.22237/jmasm/1446350640