國立成功大學

生物醫學工程研究所

碩士論文

**開發可運用於中風偏癱上肢復健之iOS擴增實境鏡像治療軟體**

**Development of iOS-based augmented reality mirror therapy software for upper limb rehabilitation in stroke-induced hemiparesis**

研究生： 黃柏瑜 Student: Po-Yu Huang

指導教授: 林哲偉 博士 Advisor: Che-Wei Lin

Department of Biomedical Engineering

College of Engineering

National Cheng Kung University

Tainan, Taiwan, Republic of China (R.O.C.)

Thesis for Master of Science

July 2023

中華民國一百一十二年七月

開發可運用於中風偏癱上肢復健之iOS擴增實境鏡像治療軟體

黃柏瑜[[1]](#footnote-1)\* 林哲偉[[2]](#footnote-2)\*\*

國 立 成 功 大 學 生 物 醫 學 工 程 學 系

# 摘 要

本論文開發了可用於中風偏癱患者復健的擴增實境鏡像治療軟體，一種相較於沉浸性虛擬實境復健系統、可直接在使用者iOS手機的方案，旨在提供傳統鏡像治療的便利性，同時回饋高沉浸的視覺刺激以提供較好的上肢復健效果。本軟體基於Apple iOS作業系統開發，由手機後鏡頭、人體語義分割神經網路與支持圖形運算加速的渲染器構成。模擬鏡像治療原理、將使用者手部輪廓影像以最高60幀的更新率即時渲染於對側視野中。本論文驗證擴增實境鏡像治療軟體成效的研究招募了三十名年輕的健康受試者參加臨床試驗，每位受試者均在前後一周的時間分別被施以一次30分鐘的傳統鏡像治療與擴增實境鏡像治療的上肢功能介入實驗，在實驗開始後的前十分鐘使用了功能性近紅外光譜，估測受試者在不同介入條件下，執行十次一分鐘捏取運動時的前額葉與運動感覺皮質區的血流灌注量；後二十分鐘執行上肢運動功能訓練，包含前臂/拇指旋轉60次、手腕/手指屈伸60次、對掌運動60次以及肌腱滑動訓練60次。評估其在抓握提取測試、普渡釘板測試、明尼蘇達手動敏捷測試、兩點距離測試以及單絲觸覺測試中的前後測表現，並使用重複測量變異數分析統計組間差異。結果發現擴增實境鏡像治療在提升手指捏取協調性、手指靈活度、上肢粗大運動以及降低兩點距離閥值的表現上，均優於傳統鏡像治療與前測基準，並且存在顯著差異。功能性近紅外光譜的測量則顯示兩種介入方式下的前額葉左右腦區之時間血流變化量，其相關係數均達0.9以上；運動感覺皮質區的相關性則分別為0.3（擴增實境鏡像治療）與0.7（傳統鏡像治療）以上。研究結果顯示該軟體具有應用在臨床居家中風上肢復健的潛力。

**關鍵字:** 鏡像治療、居家復健、擴增實境、移動裝置、遠距醫療

**Development of iOS-based augmented reality mirror therapy software for upper limb rehabilitation in stroke-induced hemiparesis**

Po-Yu Huang[[3]](#footnote-3)\* Che-Wei Lin [[4]](#footnote-4)\*\*

Department of Biomedical Engineering

National Cheng Kung University, Tainan 701, Taiwan, R.O.C.

# Abstract

This paper has developed an augmented reality mirror therapy software that can be used for the rehabilitation of stroke patients with hemiplegia. Compared with the immersive virtual reality rehabilitation system, it can be directly installed on the user's iOS mobile phone. Aiming to provide the convenience of traditional mirror therapy while giving highly immersive visual stimulation to provide better upper limb rehabilitation. This software is developed based on the Apple iOS operating system, and consists of a mobile phone rear camera, a human body semantic segmentation neural network, and a renderer that supports graphics computing acceleration. Simulating the principle of mirror therapy, the contour image of the user's hand is instantly rendered in the contralateral view at a maximum update rate of 60 frames. Thirty young healthy subjects were recruited to participate in clinical trials in this paper to verify the effectiveness of augmented reality mirror therapy software. Each subject was given a 30-minute traditional mirror therapy in one week before and after. In the upper limb function intervention experiment with augmented reality mirror therapy, functional near-infrared spectroscopy was used in the first ten minutes after the start of the experiment to estimate the subject's blood perfusion in the prefrontal cortex and sensorimotor cortex area by performing ten one-minute pinch tasks under different intervention conditions; after 20 minutes, perform upper limb motor function training, including forearm/thumb rotation 60 times, wrist/finger flexion and extension 60 times, palm movement 60 times and tendon sliding training 60 times . The pre- and post-test performance in the Pinch-Holding-Up-Activity test, Purdue Peg board test, Minnesota Manual Dexterity test, Two-point Discrimination test, and Semmes-Weinstein Monofilament was evaluated. The differences between groups were statistically analyzed using repeated measures variance analysis. It was found that augmented reality mirror therapy was superior to traditional mirror therapy and pre-test benchmarks in improving finger pinch coordination, finger dexterity, upper limb gross movement, and reducing the distance threshold between two points, and there were significant differences. The measurement of functional near-infrared spectroscopy showed that under the two intervention methods, the correlation coefficients of the temporal blood flow changes in the left and right brain regions of the prefrontal cortex were all above 0.9; the correlation coefficients in the sensorimotor cortex were 0.3 (augmented reality mirror therapy) and above 0.7 (traditional mirror therapy). The results of the study show that the software has the potential in clinical home stroke upper limb rehabilitation.

**Keywords:** Mirror Therapy, Home Rehabilitation, Augmented Reality, Mobile Device, Telerehabilitation

# 致謝

本論文幸蒙我的導師林哲偉教授用心的指導，研究過程道阻且長，然行則將至。在兩年的短暫時日中，若無林老師的耐心與扶持，我想我將繼續如同以前的自己一樣，在遭遇到各種大大小小的阻礙後便停滯不前。在無數個討論的日子裡，您不僅以一位前輩的身分，在我遭遇困難時予我許多理論上的知識和建議；在一些身心特別脆弱的日子裡，亦時常以一位友人的觀點，引導我走出自陷的陰霾之中。師恩浩瀚，我無以為報，在此向您致上最高的敬意與謝意。

口試期間承蒙口委 郭立杰教授、徐秀雲教授以及古佳苓教授對於我碩士論文內容的細心指正與諸多在專業復健領域的寶貴意見，這些幫助使本論文更臻完善。在此，我需要特別感謝徐秀雲老師與她的助理育婷學姊，於研究期間協助了我部份的實驗設計、介入流程以及數據的分析。在實驗器材的選用上，也感謝成大醫工所 蘇芳慶教授，以及於蘇教授動作分析實驗室的馬千里學長同意租借貴重儀器予我使用在受試者實驗中。

復健系統開發期間，感謝台南好想工作室的工程師 Jeremy協助軟體上架於官方平台的相關事宜，並在軟體開發技術層面上的傾囊相授；感謝遠在海外素未謀面，熱情的自由軟體開發者 Turner，在信件來往過程中不但對於我的開發予以肯定，並無償的讓我用了他所開發的套件以完善系統內部的各項功能。

修業期間，謝謝與我一同奮鬥的好友盈真、梓豪與睿昇相互砥礪與幫助，在撰寫碩論期間，我們相互聚合成的永動機大幅度的提高了彼此撰寫論文的速度和品質。謝謝大學長侑良與行政人員雅婷、瓊瑤在生活層面上的幫忙，豐富了我的研究所生涯。

最後，感謝我的家人與伴侶從始至終無私的奉獻，因為你們的支持與鼓勵，我才能在求學過中不斷的努力進步，成為一個更好的人。

# Table of Contents

[摘 要 I](#_Toc142055838)

[Abstract III](#_Toc142055839)

[Table of Contents VI](#_Toc142055840)

[List of Tables VIII](#_Toc142055841)

[List of Figures IX](#_Toc142055842)

[Chapter 1 Overview 1](#_Toc142055843)

[1.1 INTRODUCTION 1](#_Toc142055844)

[1.1.1 Background 1](#_Toc142055845)

[1.1.2 Mirror Therapy (MT) 2](#_Toc142055846)

[1.1.3 Virtual Reality Therapy 3](#_Toc142055847)

[1.1.4 Trend of Digital Health 4](#_Toc142055848)

[1.2 LITERATURE REVIEW 4](#_Toc142055849)

[1.2.1 Rehabilitation on Stroke Patient 5](#_Toc142055850)

[1.2.2 Telerehabilitation 6](#_Toc142055851)

[1.2.3 Digital Rehabilitation 8](#_Toc142055852)

[1.2.4 The Combination of Virtual/Augmented Reality 8](#_Toc142055853)

[1.2.5 Immersive Rehabilitation via Mobile Phone 9](#_Toc142055854)

[1.2.6 Quantitative Analysis on Mirror Therapy 12](#_Toc142055855)

[1.3 OBJECTIVE 13](#_Toc142055856)

[Chapter 2 Methodology and Material 14](#_Toc142055857)

[2.1 SYSTEM DEVELOPMENT 14](#_Toc142055858)

[2.1.1 Augmented Reality Mirror Therapy System (ARMT) 14](#_Toc142055859)

[2.1.2 Hardware and Accessories 15](#_Toc142055860)

[2.1.3 System Architecture 16](#_Toc142055861)

[2.2 DEVELOPMENT PROGRESS 17](#_Toc142055862)

[2.2.1 Development Tools 17](#_Toc142055863)

[2.2.2 Hand Joints Skeleton Approach 18](#_Toc142055864)

[2.2.3 Hand Contour Approach 22](#_Toc142055865)

[2.2.4 Cardboard supported and Screen Fluency Approach 31](#_Toc142055866)

[2.3 EXPERIMENTAL DESIGN 35](#_Toc142055867)

[2.3.1 Purpose 35](#_Toc142055868)

[2.3.2 Participant Criteria 35](#_Toc142055869)

[2.3.3 Procedure 36](#_Toc142055870)

[2.3.4 Hand Function Assessment Tool 40](#_Toc142055871)

[2.3.5 Brain Area Activity Measurement 44](#_Toc142055872)

[Chapter 3 Result and Discussion 46](#_Toc142055873)

[3.1 RESULT AND COMPARISION 46](#_Toc142055874)

[3.1.1 Subjects 46](#_Toc142055875)

[3.1.2 Hand Function Evaluation 46](#_Toc142055876)

[3.1.3 fNIRS Result of ROI 53](#_Toc142055877)

[3.2 DISCUSSION 56](#_Toc142055878)

[Chapter 4 Conclusion and Future Work 61](#_Toc142055879)

[4.1 CONCLUSION 61](#_Toc142055880)

[4.2 LIMITATION 61](#_Toc142055881)

[4.3 FUTURE WORK 63](#_Toc142055882)

[References 64](#_Toc142055883)

# List of Tables

[Table 1. Recent immersive rehabilitation 11](#_Toc142055938)

[Table 2. All models that can be equipped with ARMT 15](#_Toc142055939)

[Table 3. Comparison of custom model and official segmentation model 33](#_Toc142055940)

[Table 4. The motor task in the last 20 minutes of the intervention experiment 39](#_Toc142055941)

[Table 5. The content of the upper limb tests 40](#_Toc142055942)

[Table 6. The number of statistical samples for the interventional experiment 46](#_Toc142055943)

[Table 7.1. The outcome measures in each assessment scale 48](#_Toc142055944)

[Table 7.2. P value of pairwise comparison in three conditions 49](#_Toc142055945)

[Table 8.1. Beta value of fNIRS GLM regression 55](#_Toc142055946)

[Table 8.2. P value in each condition of fNIRS GLM regression 55](#_Toc142055947)

[Table 9. Comparison in between MT, ARMT and VRMT 59](#_Toc142055948)

# List of Figures

[Figure 1. Preview of ARMT 15](#_Toc142055986)

[Figure 2. ARMT System Architecture 17](#_Toc142055987)

[Figure 3. Twenty-one hand Landmarks in Vision Framework 19](#_Toc142055988)

[Figure 4. Ideal pinhole camera model 20](#_Toc142055989)

[Figure 5. The relationship between distance Z and disparity 21](#_Toc142055990)

[Figure 6. Depth detection resulting image 21](#_Toc142055991)

[Figure 7. System diagram for ARMT 3D hand joints reconstruction approach 22](#_Toc142055992)

[Figure 8. Defects of ARMT depth estimation 23](#_Toc142055993)

[Figure 9. Common applications of deep learning in machine vision 24](#_Toc142055994)

[Figure 10. EgoHands image source containing hand contour masks 25](#_Toc142055995)

[Figure 11. Modified Unet architectures inspired by MobileNetV2 26](#_Toc142055996)

[Figure 12. Whole structure of modified Unet with MobileNetV2 backbone 27](#_Toc142055997)

[Figure 13. Deep learning training workflow 28](#_Toc142055998)

[Figure 14. The training result of the modified Unet model 29](#_Toc142055999)

[Figure 15. iOS Core ML model conversion workflow 30](#_Toc142056000)

[Figure 16. Multiple layers defined in GUI 30](#_Toc142056001)

[Figure 17. System diagram for ARMT Hand Contour Approach 31](#_Toc142056002)

[Figure 18. Limited ARMT application scenarios 32](#_Toc142056003)

[Figure 19. The figure occlusion indication shown at the ARKit3 conference 33](#_Toc142056004)

[Figure 20. System diagram for final version of ARMT system 35](#_Toc142056005)

[Figure 21. Flow chart of the clinical trial in healthy subjects 36](#_Toc142056006)

[Figure 22. MT condition mirror box (left) and ARMT condition (right) 37](#_Toc142056007)

[Figure 23. fNIRS position map 38](#_Toc142056008)

[Figure 24. Block design of the experiment for each condition 38](#_Toc142056009)

[Figure 25. Subjects in fNIRS intervention 38](#_Toc142056010)

[Figure 26. PHUA test 41](#_Toc142056011)

[Figure 27. Purdue Pegboard test (PPT) 42](#_Toc142056012)

[Figure 28. Semmes-Weinstein Monofilament test (SWM) 42](#_Toc142056013)

[Figure 29. Two-point Discrimination Test (2PD) 43](#_Toc142056014)

[Figure 30. Minnesota Manual Dexterity Test 44](#_Toc142056015)

[Figure 31. Pre-processing flow in Homer3 45](#_Toc142056016)

[Figure 32. Processed fNIRS signal preview 45](#_Toc142056017)

[Figure 33.1. Chart result of PHUA 50](#_Toc142056018)

[Figure 33.2. Chart result of PPT 51](#_Toc142056019)

[Figure 33.3. Chart result of 2PD test 52](#_Toc142056020)

[Figure 33.4. Chart result of MMDT 52](#_Toc142056021)

[Figure 34. fNIRS channels covering functional cortex 53](#_Toc142056022)

[Figure 35. Trends in HbO during the intervention 54](#_Toc142056023)

[Figure 36. Interquartile range of beta value in ARMT and MT intervention 56](#_Toc142056024)

[Figure 37. The quality of signal acquisition is unstable to each subject 57](#_Toc142056025)

[Figure 38. Existing MT Concept Rehabilitation APP 60](#_Toc142056026)

# Chapter 1 Overview

## INTRODUCTION

## 1.1.1 Background

For post-stroke survivors, the most common sequelae are hemiplegia which is a type of paralysis that affects one side of the body, cause a range of physical impairments, including weakness, spasticity, and loss of sensation, and significantly impact a person's ability to perform daily activities. Stroke can cause a decrease in functionality in various ways, depending on the affected brain region. However, the most common and frustrating defects are related to motor and sensory impairments, which often occur in groups of survivors. From the estimates of the frequency of the impairments on admission for rehabilitation 70-85% stroke patients suffered by hemiplegia [1]. Hence, upper limb rehabilitation is a critical practice for stroke survivors to regain functional independence and improve their quality of life. Including grasp, reach, dexterity, and coordination, the importance of upper limb rehabilitation is such that many routine rehabilitation exercises mostly include their program.

Reports from clinical and therapist experiences, most scholars agree that rehabilitation after stroke has a decisive impact on patients' prognosis. Rehabilitation quality, immediacy, duration, and patients' adherence are crucial factors that directly affect post-stroke survivors' maximum recovery potential. Rehabilitation aims to help stroke patients regain their general life skills. Upper limb rehabilitation, which focuses on recovering patients' arm, shoulder, hand, and wrist, is an essential part of the overall rehabilitation process. Not only is it complex to control, but human upper limbs also play a critical role in daily activities, such as self-care, intake, dressing, and working. The early and intensive upper limb rehabilitation can improve outcomes for stroke survivors, including better functional outcomes and restore the life quality before the stroke to the greatest extent. Hence, upper limb rehabilitation is considered a critical component of stroke rehabilitation, and it is often prioritized over other forms of rehabilitation.

Theoretically, based on the systematic rehabilitation schedule and consistent practice with a therapist, most minor stroke patients can achieve complete recovery within six months. Although extensive stroke patients may require several years and may not fully recover, early exposure to therapy is critical during the recovery process. Therefore, balancing the quality of therapy and creating an interesting and immersive experience to support their willingness to participate has become a significant topic of research.

In the recent years, there has been growing interest in innovative rehabilitation methods that incorporate technology, such as virtual reality and robotics, to enhance the effectiveness and efficiency of stroke rehabilitation. These methods offer potential advantages such as increased patient engagement, personalized feedback, and improved outcomes.

Canadian Stroke Best Practice Recommendations lists several rehabilitation methods that have a lot of evidence to support their effectiveness [2]: functional electrical stimulation, mirror therapy and virtual reality therapy. Whether these upper limb rehabilitation methods are implemented in the early or late stage of stroke, they have obvious curative effects in more than two randomized controlled clinical trials.

## 1.1.2 Mirror Therapy (MT)

Mirror therapy is a type of therapy that is used to release phantom limb pain and improve motor function in stroke patients, especially suitable for stroke patients with hemiplegia [3]. In a traditional mirror therapy treatment, the therapist will ask the patient sitting in front of the mirror box and hiding their affected hand into that mirror box, on the other healthy hand will be asked to place outside of the mirror box, by adjusting the angle between the patient's perspective and the mirror on the mirror box, a affected hand image reflected by the healthy hand will show up in the mirror and create a visual illusion that tricks the brain into thinking that the missing or injured limb is functioning normally, performing the same movement with the healthy hand.

After a stroke, patients may experience a phenomenon called learned non-use, where they avoid using their affected limb because it feels weak or unresponsive. This can lead to further deterioration of motor function and make it more difficult to recover. By using a mirror to create an illusion of movement in the affected limb, mirror therapy can help to overcome learned non-use and promote recovery of motor function. The visual feedback provided by the mirror can help to retrain the brain and encourage patients to use their affected limb more actively. For a treatment based on visual deception, its efficacy is believed to be related to mirror neurons and neuroplasticity principles derived from the human brain.

The basis of mirror therapy is based on the neuroplasticity of the brain which can be repaired by itself. If the patient after the stroke keeps looking at the weak side of the hand, and constantly inputting negative information to the brain, it will not be conducive to the repair of the brain. Therefore, the mirror is used to reflect the unaffected hand, so that the patient sees the image of the unaffected hand overlapping the affected side of the hand and establishes the visual illusion of the affected side in the brain.

## 1.1.3 Virtual Reality Therapy

Virtual reality (VR) therapy is a type of digital therapeutic that will be interpreted in subsection **1.2.4 The Combination of Virtual/Augmented Reality**. The therapy uses virtual reality technology to simulate real world-like environments to help patients overcome a variety of physical, emotional, or psychological challenges. VR therapy can be used in a range of settings, including occupational therapy, physical therapy, and mental health therapy. Depending on the use case, research in VR therapy is broadly divided into immersive VR therapy and non-immersive VR therapy. Immersive VR therapy typically involves a headset/goggle that immerses the user in a computer-generated environment. non-immersive VR therapy, on the other hand, uses a flat display or projection to achieve a similar effect, and the user will still have part of his visual perception exposed to the real world.

By interacting with this virtual environment in a variety of ways, and using hand-held controllers or other devices, the VR experience can be adjusted to meet the specific needs and goals of the individual, and the therapist can guide and monitor the therapy session in real-time. Most of the VR training course can be designed and developed by software engineers, and can be adjust according to different needs, and different users [4, 5]. A well-designed immersive VR therapy system can combine with another therapy practice, but more entertaining and fulfilling, which is an advantage for stroke patients who need to undergo rehabilitation for a long period.

## 1.1.4 Trend of Digital Health

According to the World Health Organization’s (WHO) definition in Global Strategy on Digital Health 2020-2025, digital health expands the concept of eHealth to include digital consumers, with a wider range of smart and connected devices. It also encompasses other uses of digital technologies for health such as the Internet of Things (IOT), advanced computing, big data analytics, artificial intelligence including machine learning, and robotics [6]. Contrast to adopting healthcare workers, digital health refers to the use of technology to support and enhance healthcare services, including the delivery of therapy, evaluate, and scheduler systems. Digital health can help to reduce healthcare costs by streamlining administrative tasks, improving efficiency, and reducing the need for in-person visits. This can lead to cost savings for both healthcare providers and patients.

Digital therapeutics have made surprising progress since the evolution of the edge device cause in most of the cases. One example of the application is real time physiological signal monitor, the therapy of chronic disease patients has a high dependency with their lifestyle and behavior changes, by utilizing low-cost devices nearby, physiological signals in time can be detected, collected, and evaluated by patients and the medical assistants.

On the other hand, telemedicine is a form of healthcare that allows healthcare providers to communicate with their patients remotely by using several communication technologies. Post pandemic era has revealed the potential for telemedicine to improve access to healthcare for patients in remote or underserved areas, or for those who have difficulty accessing traditional healthcare services for various reasons.

## 1.2 LITERATURE REVIEW

To confirm the principles of the existing rehabilitation methods, in the literature research, this study focuses on stroke rehabilitation based on the principle of neuroplasticity. Since stroke rehabilitation requires high-frequency implementation, the literature on home rehabilitation and digital medicine will also be included. Finally, we found that many rehabilitation assessments are limited to subjective data such as scales. We also discuss the literature that quantifies brain signal changes as an assessment method.

## 1.2.1 Rehabilitation on Stroke Patient

Many current rehabilitation treatments for hemiplegic stroke patients are grounded in the theory of neuroplasticity, which refers to the brain's ability to reorganize and grow by altering its neural connections over time [7]. This phenomenon involves rewiring the brain to function differently from its previous state.

Related research suggests that multisensory stimulation and explicit feedback principles should be implemented for motor-oriented rehabilitation. The consistency of action and motor intention, one or multiple sensory stimulation at the same time, is an important factor in inducing neuroplasticity [8], and this factor is also reflected in the research direction of these three effective stroke rehabilitation methods. As an indispensable role in dealing with daily life, upper limb rehabilitation training is currently the most mainstream and most researched rehabilitation goal, besides, two-thirds of the studied interventions deal with motor recovery in recent years [2].

Neuroplasticity is not a rare mechanism to human brain [9, 10]. To keep adapting different conditions, our brain is always changing. For the post-stroke patients, the mechanism of neuroplasticity let their brain try to repair itself, but since the dramatically changes of the patients’ behavior after the trauma such as reduced use of affected side and self-limitation due to disability, the nature process of these mechanism are often limited and misleading, the main objective of the stroke rehabilitation is to correct the way that neuroplasticity has taken [11].

For rehabilitation, there have several important principles, first is **Learned non-use (Use it or lose it)**. Research of the Braille readers reveals the representation in the brain have high relationship with the frequency of use of a body part [12, 13]. Under the influence of neuroplasticity, the corresponding cerebral cortex area responsible for sensory finger skin even expands and inhibits the sensory ability of other infrequently used finger skin. Hence, some of the rehabilitation method such as constraint-induced therapy (CIMT) has been proposed [14].

Second is **the motor control is taken over by bilateral hemisphere**. Despite most of the motor control are dominant by the contralateral hemisphere, there still have weak neural pathway on corresponding ipsilateral hemisphere in humans. Although controversial, these pathways may possibly be relevant in stroke recovery [15]. Hence, the best recovery seems to those treatment focus on reorganizing damaged hemisphere, but bilateral symmetrical arm movement training is also seeming to be helpful to stroke patient, especially for the hemiplegia. MT is one of the represent treatments, which was initially developed to assist patients with upper limb amputation in managing phantom limb sensation and pain, as evidenced by the literature. In 1995, scholars extended this method to stroke rehabilitation and observed significant improvements in joint activity, speed, and accuracy for patients with mild, moderate, and severe limb disability. These positive outcomes not only enhance upper limb function but also motivate patients to utilize their affected side more frequently in their daily activities [3].

Third is **multisensory input can increase the effectiveness**. Human is socialized, but the study indicated that stroke patients are frequently alone for approximately 60% of their time, and during their waking hours, they engage in physical inactivity nearly 75% of the time [16]. The ultimate goal of rehabilitation is to get patients back into daily life, including complex and stimulating social behaviors, Some studies advocate that exposing patients to multisensory stimuli, such as rehabilitation fields that include motor, sensory, visual, and tactile feedback, will help induce neuroplasticity [17, 18].

## 1.2.2 Telerehabilitation

Telerehabilitation can be a highly beneficial option for stroke patients who are willing to receive remote care. For patients with limited mobility or remote access to hospitals, telemedicine can provide a convenient and effective way for patients to receive this care without having to leave their homes. Several research had investigated the quality and patients’ adherence during the telerehabilitation. Just like the traditional treatment, the efficacy of rehabilitation decreases within 6 months, it is recommended that distance rehabilitation exercises be easy, time-consuming, adaptable, personalized or motivating [19, 20]. One systematic research also affirms the effectiveness of real-time telerehabilitation methods (where medical staff communicate with patients in real time using telephones or live streaming) in alleviating patient discomfort and improving limb mobility [21]. In plenty of the rehab methods, MT for phantom limb pain (PLP) patient is confirmed effective to be using in home, and can be conducted entirely with initiation, feedback, and follow-up with health-care professionals remotely [22].

On method-based classification, a systematic review broadly categorized telemedicine into three types, and confirms that the telerehabilitation can produce the similar outcome to traditional rehab, it also affirms the importance of cost-effectiveness in telerehabilitation [23]. First type is the **image-based telerehabilitation**, which is using computer vision to quantify patient movements to assess rehabilitation performance, with low network bandwidth requirements [24]. Another type is the **sensor-based telerehabilitation.** Using miniaturized accelerometers and gyroscopes to assess a patient's position and trajectory in 3D space is not a recent development, but few studies have combined the technology with real-time remote communication [25, 26]. The other type is **virtual environments and virtual reality telerehabilitation**. The definition of the VR telerehabilitation here is “fully immersive virtual environment”, with the use of head mounted visual displays and other sensory input devices like haptic feedback device [27], the system allows a therapist in a remote location to conduct treatment sessions using a virtual-environment-based motor-training system with a patient who is located at home. Compared to the traditional therapy, the advantages of VR therapy can let the patients experience more immersive multisensory feedback, entertainment that improves patients’ adherence and willingness during the rehab.

The above literature surveys indicate that the main axis of research on telerehabilitation is to use communication equipment to try to bring traditional rehabilitation methods into home practice; and to develop small communicable (usually Bluetooth) sensors that can track motion trajectories. Because of its simplicity and relatively good efficacy, the MT-based rehabilitation is capable for investing in routine home rehabilitation. VR rehabilitation is a relatively new research topic. Computer calculations are used to create a realistic rehabilitation environment. In addition to providing a higher sense of immersion in rehabilitation, the digital system is also capable of recording the user's performance. However, the high cost of equipment makes it difficult to put it into home rehabilitation applications.

## 1.2.3 Digital Rehabilitation

In digital rehabilitation, the development of virtual reality (VR) or augmented reality (AR) has received considerable attention [28], various advantages had been found, these including giving patients the motivation of active self-learning, measuring patients’ behavior in safe and realistic environment, and have the ability to formulate more personalized training for patients based on these data, such as dynamically increasing or decreasing task difficulty [29]. Several studies have also reported that the VR/AR participants enjoy those rehabilitation session, which can increase their motivation to exercise more frequently at home or between sessions [30, 31]. In addition to academic research, there are also many commercial cases in the current VR rehabilitation system [32].

Consider to the cost on the VR/AR equipment and the consumption level in remote regions or developing countries, some of the research topic focusing on a low-cost digital therapy system, dedicate promote the relatively immersive rehabilitation solution. These research will be discussed in subsection **1.2.5 Immersive Rehabilitation via Mobile Phone**.

## 1.2.4 The Combination of Virtual/Augmented Reality

Based on the above-mentioned advantages, VR/AR technology is often used in combination with other proven effective therapies, and different studies have demonstrated the characteristics of its rehabilitation system: Miclaus *et al*. using MIRA (non-immersive VR software) to evaluate its effectiveness of upper limb paralysis, The experimental results of 55 stroke subjects showed that the curative effect of MIRA in the six months before and after the stroke was better than that of traditional rehabilitation therapy [33]; Weber *et al*. designed a 10-subject experiment to examine the feasibility of immersive virtual reality mirror therapy for upper limb paresis after stroke, confirmed that the combination of immersive VR and MT is well-tolerated by chronic stroke patients and has preliminary evidence of efficacy [34]; CW Lin *et al*. developed an immersive virtual reality mirror therapy (VRMT) to evaluate the upper limb function of 30 healthy subjects and 45 stroke patients after using the system for a period of nine weeks. The result was that VRMT had a better curative effect than traditional MT intervention [4, 5], this study was also the longest and the second-highest number of participants compared to other immersion therapies in a systematic literature review [35]; Hoermann *et al*. evaluated the patients’ and the therapists’ opinion in a clinical feasibility study at a rehabilitation center by using self-designed AR mirror therapy system, results in the system is feasible for clinical use [36]; Gilda *et al*. utilized Electromyography (EMG) to detect the paralyzed arm moving intention from stroke patients, combining the AR technology, rendering the patient's paralyzed arm to the expected position and project it in front of the patient's eyes to provide visual stimulation, found that the range of arm abduction in 4 patients improved significantly after the intervention [37]. This method of using EMG to predict the movement intention of the user's affected hand and inputting commands into VR has also been used in the other literature [38].

## 1.2.5 Immersive Rehabilitation via Mobile Phone

Another research also aims to solve the problem that the cost of VR equipment is too high for telemedicine or personal use. A study shows that the existing VR rehabilitation systems have some limitations, making it difficult for ordinary patients to use them easily, such as relying on a pre-established static safety environment and high costs that make it difficult for individuals to afford [29].

An immersive rehabilitation system requires at least two sets of independent hardware devices, namely a head-mounted display and a high-performance computer. If we add sensors that capture position, such as the Oculus rift, at least one piece of hardware is confined to a static space, making it difficult to move the entire system, this will lead to be difficult to install and customize to meet specific user needs. As such, most VR rehabilitation systems are limited to hospitals or clinics and are only available to patients during appointments [28]. Cost is also one of the key points to consider, without considering the price of a commercial rehabilitation system, the price of additional VR equipment and computing hosts will cost at least 1,000 to 15,000 USD. For hospitals, the hardware acquisition cost of commercial and customized VR solutions may be affordable, because they can be used by multiple patients to share the cost, but for individuals, the purchase of VR rehabilitation equipment is more expensive. The costs may outweigh the benefits.

To solve this problem, Zirbel *et al*. develop a low-cost, portable, flexible, and interactive VR system called VRehab system [39]. The system uses a smartphone as a display and computing device, which uses Google Cardboard, a low-cost headset made of lens and corrugated cardboard, and Myo armband worn on the user's arm [40]. Myo armband predicts hand gestures through EMG signals and uses low-cost Bluetooth transmits the signal to the mobile phone, and then assists the user to make a series of decisions in the virtual environment. The whole thing costs just 100 to 300 USD and can be set up in 10 minutes; Based on the needs of the general stroke rehabilitation, LaPiana *et al*. has also developed an AR upper limb rehabilitation system using a mobile phone as a platform [41]. The system uses ARTag, a position marker system that can be applied in AR technology [42], to locate the position of the patient's hand to complete a series of entertaining tasks. The lack of in-depth efficacy verification in both documents suggests that research in this field is still developing and has yet to reach maturity.

Table 1. Recent immersive rehabilitation

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
| **Reference** | **Duration** | **Number of patients** | **Method** | **Significant improvement** |
| [33] | 9 months | 55 (stroke) | Non-immersive VR + Robotic gloves | **MMT, FMUE**  and **FIM** |
| [34] | 30 min × 12 | 10 (stroke) | Immersive VR mirror therapy | **FMUE**  **(Not significant)** |
| [4, 5] | 12 weeks | 30 (healthy)  45 (stroke) | Immersive VR mirror therapy | **FMUE, BBT** |
| [36] | Five-time trial | 5 (stroke) | Non-immersive AR mirror therapy | No experiment carried out |
| [37] | 4 weeks | 8 (stroke) | Non-immersive AR + EMG wristband | **FMUE** |
| [38] | 6 days | 13 (healthy) | Immersive AR + EMG wristband | Number of pins that were successfully transferred |
| [39] | One-time trial | 6 (stroke) | Immersive smartphone VR + EMG wristband | No experiment carried out |
| [41] | 1 week | 5 (stroke) | Immersive smartphone AR + ARTag anchor | No experiment carried out |

**MMT**: Manual Muscle Testing, **FIM**: Functional Independence Measure

**BBT**: Box and block test, **FMUE**: Fugl-Meyer Assessment for Upper Extremity

## 1.2.6 Quantitative Analysis on Mirror Therapy

In the current method of observing neuroplasticity, studies have found that brain-derived neurotrophic factor (BDNF) plays an important role in the mechanism of neurorestoration, and can be used as one of the quantitative indicators for judging rehabilitation status [43, 44]. Compared to the measurement of BDNF level in the blood sample, another measurement techniques are non-invasive and had been mass adopted by the research. Functional near-infrared spectroscopy (fNIRS) is a non-invasive brain imaging technique that measures changes in blood oxygenation in response to neural activity [45]. Human tissues are relatively transparent to the near-infrared light (650–1000 nm), it can penetrate the scalp and skull and reach the brain tissue, where it is absorbed by hemoglobin in the blood vessels, by measuring the changes in the absorption of this light, fNIRS can provide an indirect measure of neural activity in different brain regions. fNIRS has several advantages, such as portable, low-cost and relatively easy to access, therefore, some research related to evaluation the effectiveness of MT choose to use fNIRS as their quantitative analysis method [46, 47]. Electroencephalography (EEG) is another non-invasive neuroimaging technique, by measuring the electrical activity of the brain using electrodes placed on the scalp, EEG machine can amplify and recorded the activity of certain brain region. EEG’s advantages are high temporal resolution (ability to measure changes in brain activity over time) and its relatively low cost. However, its spatial resolution (ability to precisely locate activity within the brain) is lower than other techniques, same as fNIRS, the MT research also consider using EEG as the analysis method [48]. Functional magnetic resonance imaging (fMRI) is a neuroimaging technique that uses magnetic fields and radio waves to measure changes in blood flow and oxygenation in the brain. It provides a non-invasive and safe way to study brain activity. Though it has a best resolution of region and has ability to scan those deep functional cortical area, its enormous size, high cost, and low temporal resolution lead to its low usage in MT rehab research [49], especially in combination with digital therapy interventions, since fMRI does not allow electronics to enter its interior.

## 1.3 OBJECTIVE

As the previous literature review, some studies have found that VR-based MT is more effective in improving patients' mobility compared to traditional MT [4, 29]. However, those current research gap is the requirement of expensive equipment costs and the complicated setting process of VR equipment, which make it difficult to be effectively used in clinical fields [50]. According to statistical research, the predict of home penetration of VR equipment is only 6.3% in 2026 [51]. Blame for cost, portability and size, VR rehab system may be adopted by hospitals, but it is impractical to promote it to every patient's home. Take this as a vision, minority of the research use a smartphone as a display and computing device, also use Cardboard as an alternative VR head-mounted display [39, 41]. However, these studies were only in the preliminary stage, and their efficacy were not been tested.

In addition, how to evaluate the rehabilitation status of home rehabilitation patients will also become a problem that medical staff needs to think about. In the traditional hand-function evaluation scale, the evaluator is often required to be face-to-face with the subject before the evaluation can be performed. By recording the user, the development of digital health will bring the potential of remote assessment.

Affected by some studies that use smartphones, which are more common than VR equipment, as the carrier of immersive stroke rehabilitation systems, we decided to develop a mobile phone augmented real-time rehabilitation system based on the principle of MT, which is suitable for stroke patients in perform daily rehabilitation exercises at home with their own mobile phone and lightweight, inexpensive equipment. The system should obtain the advantage of immersive rehab feedback to ensure its superior effectiveness than MT, but preserve MT’s advantages of cost, portability and convenience.

# Chapter 2 Methodology and Material

## 2.1 SYSTEM DEVELOPMENT

## 2.1.1 Augmented Reality Mirror Therapy System (ARMT)

To solve the defects of the virtual reality mirror therapy equipment mentioned above, this study has developed a mobile device-based Augmented Reality Mirror Therapy (ARMT) system. All data processing of this system is done on a single mobile phone, but users are expected to wear a Cardboard to use (optional). This development aims to allow patients to receive immersive rehabilitation treatments only by using their own mobile device as a display instead of VR head-mounted display. The preview of ARMT is like a general camera preview but allows user to switch between camera mode or headset mode **(Figure 1)**. Under headset mode, the real-time preview screen will be split into two equivalent windows, which are specially provided for the left and right eyes of the human body, resulting in the illusion of three-dimensional feedback. Following the concept of traditional MT, the feature of this system is rendering the image of any human body to the mirror side of the screen, including but not limited to hands and arms covered with clothes. Because of referencing the user's body part as a rendering target directly, ARMT can render different and personalized illusion for each user: the texture of the skin, size, and other characteristics of the mirror fake limb would be rarely different compared to the user's real limb, whereas the background of the preview will not be influenced, this allows ARMT to provide users with more realistic visual feedback than MT, thereby increasing their immersive experience. An additional feature of the ARMT is capable of creating a custom virtual bulletin board object in the AR preview scene for users to notice any necessary information during the rehabilitation.

Figure 1. Preview of ARMT

**The preview of camera mode (left) and headset mode (middle). Wearing preview combined with cardboard (right). The left hand in all figures is illusory.**

Based on the concept of augmented reality, not like an immersive VR rehabilitation system, ARMT can adapt to various scenarios without regional restrictions, or the need to define a safe zone, because the user can still perceive the actual surrounding objects and conditions. Considering the cost, versatility, usage rate, and volume of the whole VR equipment, mobile phone-based rehabilitation systems also raise the usability of ARMT and are suitable for practicing in daily rehab training at anytime and anywhere. ARMT's screen update rate can reach a maximum of 60 frames per second (FPS) through internal hardware acceleration. Compared with VR devices, it may not be a smooth level, but it is enough to handle most of the circumstances.

## 2.1.2 Hardware and Accessories

ARMT is only available deployed on iPhones which in iOS 15 (or higher) and equipped with Apple A12 Bionic chip (or other higher end chips). **Table 2** shows the results so far ARMT is applicable to all iPhone models.

Table 2. All models that can be equipped with ARMT

|  |  |  |
| --- | --- | --- |
| Launch Year | Models | Estimate Price (USD) |
| 2018 | iPhone XS series, iPhone XR | 230 ~ 260 |
| 2019 | \*iPhone 11 series | 280 ~ 420 |
| 2020 | iPhone SE (v2), iPhone 12 series | 210 ~ 610 |
| 2021 | iPhone 13 series | 460 ~ 860 |
| 2022 | iPhone SE (v3), iPhone 14 series | 310 ~ 900 |

\*Models used for development in this study

In terms of cost, assuming that the user does not own a mobile phone that matches the model of ARMT, the rehabilitation cost of using ARMT is about 300 to 800 USD. Compare to other VR rehabilitation system, even when selecting hardware in the most economical manner possible, the custom-built system will still cost approximately 1500 to 2000 USD [39]. A Cardboard that meets the iPhone size is recommended to be used together with ARMT rehabilitation. Depending on the material or other additional accessories, the cost of the Cardboard falls between 3 to 20 USD.

## 2.1.3 System Architecture

In order to implement the application that renders the illusion mirror limb based on the appearance of target limb to the real time preview, an efficient trained neural network model for human body segmentation was incorporated into the ARMT system. The neural network model receives a fixed size of pixel buffer from image data stream captured by the smartphone camera, then tagged the set of pixels that are recognized as a part of the human body. Part of the calculation will be accelerated by the Graphics Processing Unit (GPU) and bionic chip, so-called Neural-network Processing Unit (NPU) equipped inside the smartphone, therefore the time consumption from input frame to output result is quite low.

**Figure 2** shows the system architecture flowchart of the ARMT system. The system consists of three components: smartphone, Cardboard, and the user itself. The user is responsible for performing any exercise in the field of view of the smartphone back camera, during the system activated period, the camera would continuously capture and transmit real world image frames to the ARMT system. The semantic segmentation algorithm inside the ARMT system will continue to receive these images and complete the calculation in a very short time. If there are any pixels in the frames are classified as belonging to the human body, they will be marked and transformed to mirror coordinates relative to the center line of the screen and added to the hardware-accelerated shader for rendering to the Graphics User Interface (GUI). In headset mode, the renderer will split the image into two preview images on the left and right and perform barrel distortion to match the parallax of the worn Cardboard. Finally, the lens on the Cardboard will restore the real time deformed image and provide immersive mirror visual feedback to the user's eyes.



Figure 2. ARMT System Architecture

ARMT system is developed by Swift, which is a programming language primarily used to develop native Apple applications, this makes the system extremely adaptable to any Apple devices that meet the specifications and has outstanding computing performance, but it is difficult to transplant to those smartphones with other operating systems.

## 2.2 DEVELOPMENT PROGRESS

## 2.2.1 Development Tools

Developed by Apple Inc, Xcode is an integrated development environment (IDE) that used for developing ARMT. It is specifically designed for macOS, iOS, watchOS, and tvOS app development, mainly supported programming language Swift and Objective-C. Xcode provides a wide range of tools, libraries, and frameworks to facilitate the creation of high-quality applications for Apple devices. Like any other IDE, Xcode includes a code editor that supports syntax highlighting and code completion using IntelliSense.

In actual ARMT development, Xcode allows connecting physical devices and installing the compiled code on the device. It also can monitor some performance indicators of the device when running the program, such as CPU usage, GPU usage, memory space, various thread state, FPS, and power consumption estimation. ARMT has gone through three stages of development, and its characteristics and related frameworks or algorithms will be introduced in the following chapters.

For mobile applications developed without using game engines (such as Unity, Unreal Engine), the User Interfaces (UI) framework will be the starting point of development and the backbone of the code. SwiftUI is a framework provided by Swift, it allows developers to design and develop UI with less code and in a declarative way. In the case of using Xcode, IED supports interface builder to help users directly drag the required basic elements, such as buttons and scrolls, into the view, and don't need to write any code to make. The SwiftUI framework was launched in 2019, and it is recommended that developers gradually shift their development focus to it to replace the old UI design framework UIKit. Therefore, ARMT's overall UI development will use SwiftUI.

## 2.2.2 Hand Joints Skeleton Approach

In AR development, locate the object position in the real-world coordinates is crucial before rendering. Therefore, the main objective to the start of the ARMT system is to capture the actual three-dimensional hand position. For this approach, this study has implemented it based on the combination of 2D hand joints detection algorithm and double vision disparity depth detection. Two main frameworks for developing are provided by Swift: The Vision framework and the AVFoundation framework.

The Vision framework is a powerful framework provided by Apple for performing various computer vision tasks on iOS devices. It integrates some built-in machine learning algorithm that utilizes the GPU and neural engine for fast and efficient processing of image and video data. The optimization processes images and video frames in real time, making it suitable for applications that require live analysis and interaction with the camera feed. For 2D hand joints detection algorithm, sourced from the camera feed, this study utilized a hand pose tracking Application Programming Interface (API) provided by Vision to return the two-dimensional coordinates of hand joints and maps these coordinates back to the normalized screen coordinates. This algorithm is learned based on a deep learning model and can be applied in most environments. **Figure 3** shows all 21 hand joint points that can be detected by the algorithm. Algorithms can additionally generate confidence scores from 0 to 1 for detected joints, in ARMT, only the joint points whose current confidence score is greater than 0.7 will be used.

一張含有 文字, 螢幕擷取畫面, 設計, 手 的圖片

自動產生的描述

Figure 3. Twenty-one hand Landmarks in Vision Framework

Being widely exist in the organisms on Earth, binocular vision is often accompanied by fusion of vision, although the scene captured by two eyes is similar, the pupillary distance result in a slight difference between the object we saw. This disparity of two images is called parallax, which is one of the stereo vision principles for organisms. Based on the stereoscopic effect produced by binocular parallax, we have the ability to estimate the depth from the camera to the target object by the same scene captured by two cameras mounted parallel. The AVFoundation framework is responsible for operating and setting up the camera. In some models of iPhone, there are more than two camera lenses enables double vision disparity depth detection implementation possibility.

一張含有 螢幕擷取畫面, 黑色, 黑暗 的圖片

自動產生的描述

Figure 4. Ideal pinhole camera model

**Figure 4** shows the explainable model of dual parallel stereo cameras **C** and **Cʹ**, **Z** is the distance between the target object **P** in the real world and the camera. The distance **B** between the cameras is called the baseline, and **ƒ** is the focal length of the two cameras. Under the premise of fixed baseline and focal length, by triangulation, if we know the pixel points at which positions the target objects are mapped to for the individual two cameras, that is, and ,the following equation will hold:

|  |  |
| --- | --- |
|  | (1) |

In (1), the distance between the target and the cameras **Z**, which is also called depth. For the convenience of description, is called disparity. **Figure 5** intuitively describe the inverse relationship between disparity and depth. When the distance of the target is getting farther, the resulting disparity will be become smaller until it is difficult to estimate, and theoretically it will reach the limit when the disparity is less than one pixel for the lower resolution camera. Likewise, objects should not be too close to the camera, or it would cause over estimation.

一張含有 螢幕擷取畫面, 文字, 字型, 設計 的圖片

自動產生的描述

Figure 5. The relationship between distance Z and disparity

According to the description in the iOS developer manual [52], A disparity map provided in the AVFoundation framework describes normalized shift values for use in comparing two images. The value for each pixel in the disparity map is in units of 1/meters. Using the actual iPhone 11 for verification, it is found that the depth map generated by it can stably and correctly represent the actual distance between the object and the camera at a depth of 20 cm to 80 cm. This range is enough to be used in ARMT's first-person view hand coordinate detection **(Figure 6)**.

一張含有 室內, 牆, 鏡子, 螢幕擷取畫面 的圖片

自動產生的描述 一張含有 文字, 螢幕擷取畫面, 視訊, 多媒體 的圖片

自動產生的描述

Figure 6. Depth detection resulting image

**Camera preview (left) and depth map preview (right).**

**Figure 7** shows the full diagram of hand joints skeleton approach of the ARMT development progress. With multiple back cameras iPhone model, ARMT could capture the three-dimensional space coordinates of the hand in real time. using the multi-tread execution method to ensure that the hand detection algorithm based on the neural network model will not drag down the screen update rate.

一張含有 文字, 螢幕擷取畫面, 軟體 的圖片

自動產生的描述

Figure 7. System diagram for ARMT 3D hand joints reconstruction approach

## 2.2.3 Hand Contour Approach

Several problems aren’t solved in the first approach of the ARMT system development. Including enhance the realistic mirror hand visual feedback like traditional MT, lack of rendering a skeleton and the most serious defect: unreliable 3D predicted coordinates. **Figure 8** shows an inevitable object occlusion can easily make thumb or other fingers’ 3D reconstruction difficult in-depth detection algorithms that can only be computed from a single direction of sight to avoid reducing the portability of the ARMT system.

一張含有 文字, 手套, 顯示 的圖片

自動產生的描述

Figure 8. Defects of ARMT depth estimation

For these purposes, the following development of ARMT system has focused on trying to render an indistinguishable fake mirror hand into the 2D GUI rather than reconstruct the whole hand model into the real world. The users’ hand in the camera feed is the perfect material as a reference. According to the concept of traditional MT, the healthy hand of the patient will be the basis for driving the affected hand. If there is an algorithm that can distinguish the outline of the hand from the background in the image, it will be able to reproduce the realistic affected hand to the mirror side of the preview screen without affecting the presentation of the background like traditional MT.

The study introduced the semantic segmentation neural network model to achieve the above requirements. Semantic segmentation is a field of computer vision that aims to solve the image segmentation problem [53], especially the background/foreground classification. There are several common techniques that be used to implement in practice, such as Otsu algorithm [54] and balanced histogram thresholding [55], these algorithms are based on the image histogram in the classic computer vision image processing. In ARMT’s requirement, the real time hand contour segmentation practice can be seen as a particular case in background/foreground image segmentation. However, it is hard to simply solve it by introducing these segmentation algorithms based on fixed condition judgment. Patients’ skin texture, the color similarity of the hand to the tabletop, and various changing backgrounds of the real world during the rehabilitation training would dramatically influence the stability of such algorithms. On the other hand, the rapid growth of deep learning and the rise of the hardware computing level supplies another solution to the image segmentation problem. In several implementation methods of image segmentation, semantic segmentation is a supervised deep learning algorithm to train the model to perceive one or multiple classes of objects in an image, aiming to classify each object at the pixel-wise level **(Figure 9)**.

一張含有 狗, 狗飼養, 螢幕擷取畫面, 草 的圖片

自動產生的描述

Figure 9. Common applications of deep learning in machine vision

To train a hand contour segmentation model for the ARMT system, for the training material, this study selected EgoHands dataset [56], several reasons remaining: **1)** The dataset selects 48 different scenario that enriches background diversity, such as indoor office, yard, and outdoor table etc. This will help to train the model for all possible rehabilitation environments as much as possible. **2)** Totally 4800 image frames labeled pixels of hands appeared in the scene in detail, which is the recorded film of two-person interaction (observer and someone in front of the observer). Basically, each of the images consists of at most four hands: both observer’s and someone’s right and left hand, pixels belonging to each of the hands can be chosen to select or ignored by the developer. These give the trained model potential to semantically distinguish between the observer’s hands and someone’s hands, as well as left and right hands. **3)** Using the first-person perspective (observer perspective) to film the images, which is suit for the use of ARMT’s scenario. Because by default, the camera of the ARMT system should be consistent with the user's position and line of sight.

It's worth noting that EgoHands dataset doesn't include gestures, but any outlines of movements that might be made by the hand. In 48 different scenarios, the observer and someone are enjoying some activity like playing cards, chess, and puzzles without being instructed to constrain their hands in a certain gesture **(Figure 10)**.

一張含有 室內遊戲和運動, 圖板遊戲, 桌遊, 遊戲 的圖片

自動產生的描述

Figure 10. EgoHands image source containing hand contour masks

The semantic segmentation neural network model deploys on ARMT system need to balance high accuracy and response speed in limited hardware equipment, that is, generate corresponding hand contours promptly based on the image frames provided by the camera. As a lightweight network model, Unet was proposed in 2015 and was originally used to perform fast medical image segmentation at the cell level [57], because of its simple architecture and efficient performance, it has now become one of the classic semantic segmentation models. On a modern GPU, Unet has the ability to complete the segmentation of several images in one second. For this reason, the study introduces a modified Unet structure neural network attempting to approach the requirement, which backbone introduces the concept of MobileNetV2 [58]: inverted residuals, linear bottlenecks and depth-wise convolution **(Figure 11)**. According to theory, Unet using this Convolution Neural Network (CNN) structure inspired by MobileNetV2 can reduce the amount of calculation by about 8 to 9 times while maintaining the segmentation accuracy compared to the conventional CNN if both of their CNN kernels are 3x3.

一張含有 文字, 螢幕擷取畫面, 圖表, 數字 的圖片

自動產生的描述

Figure 11. Modified Unet architectures inspired by MobileNetV2 [58]

Using transfer learning technique, we applied the MobileNetV2 model and pre-trained parameters in the timm library to reconstruct the CNN part of Unet to boost the training progress. For the structure of the model is follow the Unet design, 4 down/up sampling in the encoder and decoder part respectively, and those output 4 sets of convolution feature maps number are 96, 32, 24 and 16. Finally, the input dimension of the model is a 224 x 224 x 3 RGB image, which is also the highest resolution that MobileNetV2 can set, and the output is a 112 x 112 x 3 RGB image for the hand contour mask **(Figure 12)**.

一張含有 文字, 螢幕擷取畫面 的圖片

自動產生的描述

Figure 12. Whole structure of modified Unet with MobileNetV2 backbone

The process of training the model shows in **Figure 13**, it has been divided into three steps. The first step is data preprocessing. In each epoch, 4,800 EgoHands images are randomly split into a training set of 4,000 images and a verification set of 800 images, and these images will pass random image filter with rotation, horizontal flip, gamma correction, and shifting pixel value based on RGB and HSV color spaces.

一張含有 文字, 螢幕擷取畫面, 字型, 設計 的圖片

自動產生的描述

Figure 13. Deep learning training workflow

The second step is to train the model, repeat the training for 200 epochs, and update the parameters in the model by calculating the loss between the source image and the ground truth. The loss function formula is as follows:

|  |  |
| --- | --- |
|  | (2) |

Where is dice loss, X is the output result and Y is the corresponding ground truth, The total of dice loss will be between 0 and 1, 0 means that the output result and the ground truth are completely coincident, and 1 means that the two have no intersection at all **(Figure 14)**.

一張含有 文字, 螢幕擷取畫面, 人員 的圖片

自動產生的描述

Figure 14. The training result of the modified Unet model

**The minimum dice loss occurs at the 140rd epoch ().**

The final step of the process is transforming the trained hand contour segmentation model into the format that can be used by the iOS system. CoreML and CreateML are the frameworks provided by Apple that can deliver fast performance on Apple devices with easy integration. CoreML provides several built-in deep learning models for different task including vision, Natural Language Processing (NLP) and sound recombination. CreateML, on the other hand, allowing developers to use third party library to train their custom deep learning model for other applications by using CoreML Converters. As a general-purpose neural network archive format packaged for iOS, the “.mlmodel” file interface can easily preview the outcomes of the model and understand its performance right in Xcode **(Figure 15)**.

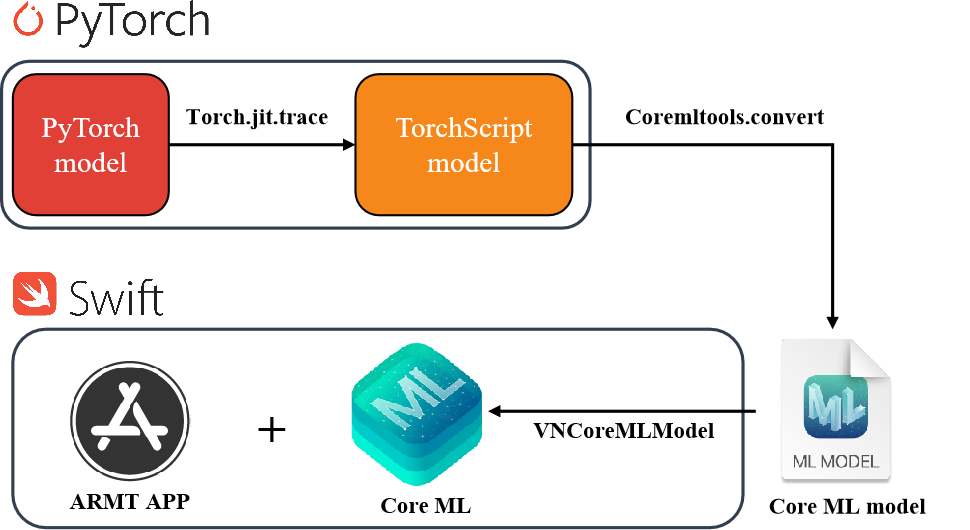


Figure 15. iOS Core ML model conversion workflow

The concept of rendering related hand contour to the mirror side of the iPhone screen is masking **(Figure 16)**. In SwiftUI design, GUI preview consists of multiple layers of view, these views are sequentially stacked on the GUI and can be masked by their upper view layer and only be shown on the region where the upper view is transparent. After the conversion of CoreML converter, each of the output pixel types from the trained hand contour segmentation model contains four bytes that represent its RGB color value, and the last byte represents transparency. By modifying these values, image frames that only extract the pixel of users’ hand are generated.

一張含有 螢幕擷取畫面, 文字, 手指, 手 的圖片

自動產生的描述

Figure 16. Multiple layers defined in GUI

**Figure 17** shows the full diagram of hand contour approach of the ARMT development progress. Since this algorithm does not rely on the depth map, it is also suitable for those iPhones that do not have multiple cameras.

一張含有 文字, 螢幕擷取畫面, 軟體 的圖片

自動產生的描述

Figure 17. System diagram for ARMT Hand Contour Approach

## 2.2.4 Cardboard supported and Screen Fluency Approach

The hand contour approach has greatly improved the fineness of the mirrored hand in the screen preview, but there are still some problems to be solved in practice: Although a neural network model suitable for building on the mobile terminal is selected, it still takes a lot of time to acquire image frames and generate masks; In terms of masking hands, the multi-layer graph stacking method was originally applied to a polygonal mask that does not change over time, and the memory is dynamically allocated to occupy the mask one by one to meet the needs of optimizing rendering efficiency. Forcibly using irregular contours that change every frame will cause frequent dynamic memory allocation and free in a short period of time, which will have a lot of computing costs. There is a strict sequential relationship between the two, and it is difficult to use parallel computing to reduce time costs, which makes the screen update rate of ARMT insufficient. In addition, compared with VR head-mounted displays, ARMT still lacks a good sense of immersion **(Figure 18)**, and cannot be placed on Cardboard for use. It is necessary to rendering the preview that provides the left and right eyes view simultaneously to solve the current problem.

一張含有 人員, 室內, 牆, 服裝 的圖片

自動產生的描述

Figure 18. Limited ARMT application scenarios

**Rehabilitation of the ARMT system without Cardboard is far inferior to that of VR head-mounted helmets.**

To solve the problem of poor performance of the custom neural network on mobile phones, we cite the official human body segmentation model provided by Apple to replace the existing hand contour segmentation model. ARKit is a framework that provides various API for AR experience, including Real-world environment perception, plane detection, creation of virtual object anchors, and label recognition. ARKit3 released in 2019 and added support the human body segmentation API for rendering the occlusion relationship between characters and AR objects **(Figure 19)**.



Figure 19. The figure occlusion indication shown at the ARKit3 conference

Although it is hard to peek at the internal algorithm implementation, it is certain that deep learning technology is also used. The algorithm is very likely to adopt the DeepLabV3 [59] architecture with MobileNetV2 as the backbone of CNN [60], and optimize it according to the internal computing chip architecture. According to the official statement, the method provided by this API produces a very short masking time, which can make sure the program runs smoothly at 60 FPS. This statement has also been confirmed by actual tests **(Table** 3**)**.

Table 3. Comparison of custom model and official segmentation model

|  |  |  |
| --- | --- | --- |
| **iPhone 11** | **Custom ML** | **Official ML** |
| **Operation time** | 35 ~ 40 ms | 10 ~ 20 ms |
| **FPS** | 25 ~ 28 | 50 ~ 100 |

On the issue of how to render the dual-view preview screen to support the use of the ARMT system on the Cardboard, we quoted the third-party package ARHeadsetKit, which is an open-source project that encapsulates ARKit and efficient rendering methods [61]. ARHeadsetKit uses Metal frameworks and Single Instruction Multiple Data (SIMD) API for efficient rendering. Metal is the framework provided by Apple to developers to directly access the GPU and can schedule and manage the rendering pipeline according to the usage situation. Metal's memory debugger can maximize the coordination of the workload of the CPU and GPU on rendering graphics, greatly reducing their idle time.

In the rendering task, Metal can manage a piece of memory called frame buffer for the CPU and GPU to share, split the workload required to render one frame into multiple draw calls, and allocate two hardware according to the amount of calculation. In Metal development, shader and texture refer to the programmable stages and image data in the rendering pipeline, respectively. Shader is used to define the various stages in the rendering pipeline, such as vertex shader and fragment shader, which are responsible for processing geometry and rasterization. Texture is used to store image data, which can be used as the input of shader to provide texture, color and other image information for rendering. Compared with the multi-layer stack rendering provided by SwiftUI, Metal tends to use shaders to perform a series of rendering processing for a single texture and push the completed material to the frame buffer for display, this can reduce large amount of dynamic memory allocation and free. In addition to coordinating the workload between hardware, the rendering efficiency is greatly improved.

**Figure 20** shows the full diagram of the latest version ARMT system. The work of the shader pipeline is managed by Metal, which can be allocated to the CPU or GPU in a reasonable proportion for concurrent operations (about 2:8) and share the memory of the frame buffer address.



Figure 20. System diagram for final version of ARMT system

## 2.3 EXPERIMENTAL DESIGN

## 2.3.1 Purpose

To identify the difference in treatment effects between ARMT and traditional mirror therapy, this pilot experiment is designed to investigate the difference in immediate effects on upper limb performance of the hands between receiving ARMT and MT intervention among healthy subjects. Since MT already had many literatures and experiments to prove its effectiveness in stroke rehabilitation, the ARMT, as the innovative rehabilitation method inspired by MT, needs to show the corresponding evidence in practical circumstances. The whole process of the experiment was held by the therapist from department of rehabilitation in NCKU hospital and the thesis author.

## 2.3.2 Participant Criteria

The subjects would randomly divided into two groups and be asked to undergo two one-session interventions. The subjects recruited in this experiment should have no current or past history of neuromuscular or orthopedic problems in the upper extremities. Both groups received 30 minutes of ARMT or MT rehabilitation, after the one-week wash-out period, changing intervention groups respectively **(Figure 21)**. Before receiving the intervention, all of the subjects must be evaluated their upper limb functionality by the therapists as a pre-test.

一張含有 文字, 螢幕擷取畫面, 圖表, 行 的圖片

自動產生的描述

Figure 21. Flow chart of the clinical trial in healthy subjects

## 2.3.3 Procedure

The MT condition (with a mirror box) or ARMT condition (including an iPhone and a VRG headset) were deployed in the experiment **(Figure 22)**. For all healthy subjects, they were told to sit on a chair and placed both of their hands on the table, and their right hand was instructed to stay still. This is for the purpose of regarding right hand side as an affectation of stroke patients’ hemiplegia side.

一張含有 人員, 牆, 室內, 服裝 的圖片

自動產生的描述 一張含有 人員, 室內, 小工具, 手腕 的圖片

自動產生的描述

Figure 22. MT condition mirror box (left) and ARMT condition (right)

During the first 10 minutes of intervention, NIRScout (fNIRS, NIRx Medical Technologies, Glen Head, NY, USA) equipment was used to collect the changes in oxyhemoglobin in specific brain cortex regions of the subject, with a total of 16 detectors and 8 sources, arranged in an array 3 cm apart and distributed over the upper scalp of the motor cortex and prefrontal cortex **(Figure 23)**.The position refers to the channel position established by other literature that use fNIRS as MT efficacy analysis. For MT experiments, hand movement must be involved, so almost all literatures will choose the motor cortex on both sides. In addition, some literatures want to observe the sense of coordination and immersion of MT subjects through fNIRS or fMRI. For this purpose, the prefrontal cortex is usually selected as the observation Region of Interest (ROI) [47, 49, 62, 63]. The experiments in both MT and ARMT conditions were arranged in a 1-minute block design repeated 10 times, including the first 30 seconds rest stage with eyes closed for the purpose of given a blood perfusion baseline and the last 30 seconds of finger pinching trials, an audio clue indicates the subjects to open and close their hand, perform 2 times of pinches in 1 second **(Figure 24, 25).** In the last 20 minutes of intervention, subjects will be instructed by a professional therapist to continue performing repetitive movements for hand rehabilitation while using MT or ARMT **(Table 4)**. After the whole 30-minute intervention experiment, the subjects will immediately receive the hand function assessment post-test.



Figure 23. fNIRS position map

**Arrangement of fNIRS source (red) and detector (blue) channel (top view of subject’s head).**



Figure 24. Block design of the experiment for each condition

一張含有 人員, 服裝, 室內, 傢俱 的圖片

自動產生的描述 一張含有 地板, 室內, 人員, 足部穿著 的圖片

自動產生的描述

Figure 25. Subjects in fNIRS intervention

**MT condition (left) and ARMT condition (right).**

Table 4. The motor task in the last 20 minutes of the intervention experiment

|  |  |
| --- | --- |
| 一張含有 腳趾, 人員, 指甲, 赤腳 的圖片  自動產生的描述 | 一張含有 人員, 指甲, 手指, 赤腳 的圖片  自動產生的描述 |
| **Forearm pronation/supination × 60** | **Wrist stretch/flexion × 60** |
| **一張含有 人員, 手, 手指, 指甲 的圖片  自動產生的描述** | **一張含有 人員, 手指, 手, 指甲 的圖片  自動產生的描述** |
| **Thumb rotation × 60** | **Thumb and little finger face to face × 60** |
| **一張含有 手, 指甲, 人員, 手指 的圖片  自動產生的描述** | **一張含有 指甲, 手, 手指, 人員 的圖片  自動產生的描述** |
| **Thumb extension/flexion × 60** | **Finger extension/flexion × 60** |
| **一張含有 指甲, 手, 腳趾, 手指 的圖片  自動產生的描述** | |
| **Tendon slip × 60** | |

## 2.3.4 Hand Function Assessment Tool

For the outcome measurements, several standardized upper limb tests are used to be pre- post-test assessment tools such as Pinch-Holding-Up-Activity (PHUA), Purdue Pegboard test (PPT), Semmes-Weinstein Monofilament (SWM), Two-point Discrimination Test (2PD), Minnesota Manual Dexterity Test (MMDT). These assessment criteria will be assessed by a professional occupational therapist. **Table 5** organized the type of functions each standardized upper limb test represents, each of these will be described below.

Table 5. The content of the upper limb tests

|  |  |  |
| --- | --- | --- |
| **Abbreviation** | **Category** | **Index** |
| **PHUA** | Hand strength coordination | 1. Ratio of max pinch force and load force  2. Percentage of maximal pinch strength |
| **PPT** | Finger dexterity | 1. Pins insertion count 2. Pins assemble count |
| **SWM** | Finger sensitivity | 1. Touch-pressure threshold |
| **2PD** | Spatial resolution | 1. Two-point distance threshold |
| **MMDT** | Upper extremities gross motor function | 1. Time spent on placement 2. Time spent on flipping |

PHUA test is one of the tools for evaluate human hands coordination in sensory-motor coupling controll. In most of the circumstances, humans’ strength of pinching or grasping an object would passively adjust from the changing weight of current object causing by unstable weight center or acceleration, trying to found a best efficient ratio between strength and the holding object load weight. Based on this behaviour, Flanagan *et al*. had proposed the ratio of the maximum grip strength value to the maximum load value during the lifting process can be regarded as a sensitive parameter by which the generation of grip force relative to the load due to momentum can be observed [64]. The standard pinch-holding equipment of PHUA is the metal cuboid weighing 480 grams, which contains two load cells and an accelerometers to measure subject pinch strength and detect the cuboid acceleration when it moves. In the beginning of the PHUA evaluation stage, the subject will follow the instruction from the therapist to lift the metal cuboid above the desk for 5 cm and make sure only holding with their thumb and index finger on load cells in the entire process. After 5 second, according to the computer sound prompt, the subject raised the cuboid to 30 cm. Data collection takes 15 seconds in one epoch. The subjects performed a total of 3 times, resting for 1 minute each time. During the test, the subject's arm is dangling, and only pinch the object with the thumb and index finger on load cells **(Figure 26)**. The parameters include: **1)** maximum grip force value (FPPeak): the maximum pinch force (pinch force) during the ascent of the device (from 5 to 30 cm); **2)** maximum load value (FLMax): at the maximum The maximum load force during acceleration. The analyzed index includes: **1)** force ratio (FRpeak): the ratio of FPPeak to FLMax; **2)** Percentage of maximal pinch strength: peak pinch force divided by the maximal static pinch force. The lower value in FRpeak and percentage of maximal pinch strength: more precise pinch force scaling.

一張含有 人員, 室內, 牆, 服裝 的圖片

自動產生的描述

Figure 26. PHUA test

PPT is a fine fingertip dexterity test with validity and reliability. Subjects were asked to arrange pins and assemble pins with washers and collars within the limit of time. Results of unilateral (dominant and non-dominant hand) pin insertion count (30 seconds), bilateral pin insertion count (30 seconds) and numbers of assembly (1 minute) consisted in outcomes **(Figure 27)**. The higher the score, the more pins completed within the limited time, which is used as a reference to express the finger dexterity of the subject.

一張含有 人員, 室內, 牆, 女人 的圖片

自動產生的描述

Figure 27. Purdue Pegboard test (PPT)

SWM uses Touch Test Sensory Evaluators (North Coast Medical, Inc, Gilroy, CA) to test the skin pressure threshold. Nylon filaments of different thicknesses are applied to the volar skin for 1-1.5 seconds of continuous force, and the threshold is defined as three tests. The lightest stimulus with at least two correct answers. The test will be applied to the pulp of the finger. Each filament is numbered as the logarithm to the base ten of the strength of a tenth of a milligram. The smaller the value, the higher the sensory sensitivity of the subject's fingers **(Figure 28)**.

一張含有 人員, 指甲, 手指, 捲動方塊 的圖片

自動產生的描述

Figure 28. Semmes-Weinstein Monofilament test (SWM)

2PD is used for detecting the least distance between two prongs, evaluates subject is capable of discriminating two close points on a small area of skin (usually the finger pulp). The therapist uses the octagonal needled disk in **Figure 29** for testing, in which seven sides are equipped with double needles with a distance from 2mm to 8mm, and the remaining side is equipped with a single needle. Lightly poke the double-needle on the random side on the fingertips of the subject for 1 to 1.5 seconds until the subject can distinguish the minimum stitch distance from a single needle, or mistakenly regard a certain level of stitch distance as a single needle three times. The lower the value obtained for this item, the higher the spatial resolution of the subject’s fingertip.

****

Figure 29. Two-point Discrimination Test (2PD)

MMDT is a test that measures gross motor function of the upper extremities. The equipment consists of a number of round cake-shaped building blocks and two wooden boards with grooves for placing the building blocks. In this study, the subjects were asked to stand in front of the MMDT equipment to perform placing and flipping all the building blocks, and they were not allowed to move their positions again during the process **(Figure 30)**. The evaluating therapist would record the time it took to complete the placing of the building blocks and flipping all the building blocks. The less time spent, the better the subject performed on gross motor skill of upper extremity.

一張含有 人員, 食物, 室內, 檢查器 的圖片

自動產生的描述

Figure 30. Minnesota Manual Dexterity Test

## 2.3.5 Brain Area Activity Measurement

At the same time, for the sake of obtaining objective quantitative data, this research additionally collects the changes in cerebral blood perfusion to analyze bilateral motor cortex and prefrontal cortex activation via fNIRS when intervention begins. In terms of quantitative data, uses Homer3 [65] to remove signal artifacts, a band-pass filter (0.01~0.1 Hz) to remove physiological signals that may affect (heart rate, respiratory, etc.), and finally output the changes in oxyhemoglobin after 10-block average in the specific cortex **(Figure 31)**. It is worth noting that the process of converting optical density to concentration in the fNIRS pre-processing process is based on the Modified Beer-Lambert Law (MBLL), which is commonly used in fNIRS to convert changes in optical density to changes in hemoglobin concentration. The MBLL is an adaptation of the Beer-Lambert Law, which describes the relationship between the absorbance of light by a medium and the concentration of the absorbing substance. HbO (oxygenated hemoglobin) is typically measured using near-infrared light in the range of approximately 650 to 900 nm. This wavelength range is commonly referred to as the "near-infrared window" because it allows light to penetrate biological tissues, including the human skull, with relatively low absorption and scattering. In this experiment, we choose 850 nm near-infrared light to the source to detect HbO in the certain region of cortex.

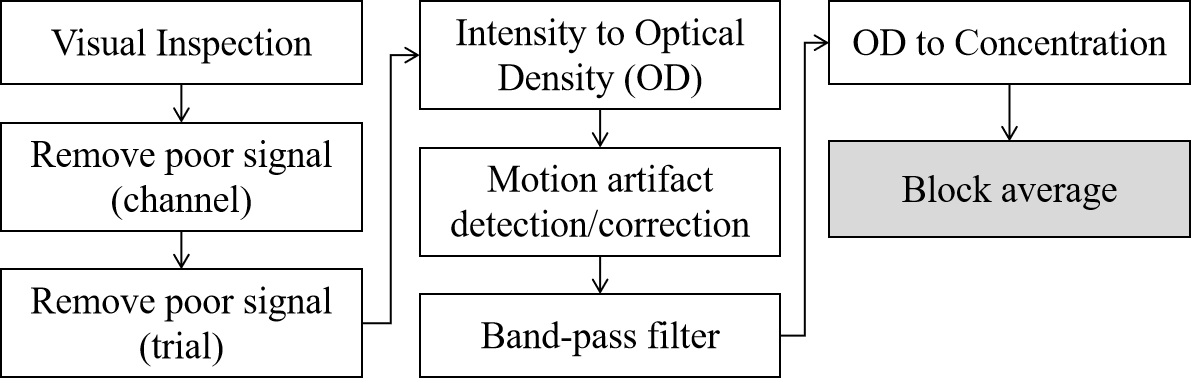


Figure 31. Pre-processing flow in Homer3

The General Linear Model (GLM) of the modified gamma function convoluted square wave according to the time length of the intervention interval was also applied for effect estimation, according to assumptions, the beta value (*β*) generated by GLM indicates the strength of the modulation of the hemodynamic response [46, 63, 66, 67]. In fNIRS quantitative analysis, GLM regression can be regarded as a method to normalize the signal of each channel, and beta value is its amplification factor. This value can be used as indirect evidence for the activation of the relevant brain area.

**Figure 32** shows one of the subjects exercised the prefrontal cortex contralateral to the motion hand (left hand) during the ARMT intervention. The processing methods of 10-block averaging and GLM regression will get different signal waveforms, but generally they will all conform to the general trend of channel strength. Channels are considered a higher excitation level will have larger beta values in GLM analysis.

一張含有 文字, 螢幕擷取畫面, 繪圖, 圖表 的圖片

自動產生的描述

Figure 32. Processed fNIRS signal preview

**Four channels of the results after fNIRS signal preprocessing in 10 intervention blocks (a), block average result (b) and GLM regression result (c).**

# Chapter 3 Result and Discussion

## 3.1 RESULT AND COMPARISION

## 3.1.1 Subjects

30 subjects (17 males, 13 females) with the mean age of 23.0 ± 2.7 years old were recruited and had experienced 30 minutes of intervention in both MT group and ARMT group and used for statistical analysis by their consent. The statistical analysis will be divided into two parts, comparing the differences between the pre- and post-tests with the scores measured by the same hand function assessment tools, that is, PHUA, PPT, SWM and MMDT introduced in subtitle **2.3.4 Hand Function Assessment Tool**. The second part is fNIRS analysis in the bilateral motor/prefrontal cortex during the MT or ARMT intervention. However, for poor signal quality in brain cortex ROI recorded by fNIRS, 5 subjects were excluded in the fNIRS analysis, also 1 subject who reported feeling 3D dizzy when using ARMT system was excluded **(Table 6)**.

Table 6. The number of statistical samples for the interventional experiment

|  |  |  |
| --- | --- | --- |
| **Category** | **Group** | **Samples (*n*)** |
| **Hand function evaluation** | MT | 30 |
| ARMT | 30 |
| **fNIRS analysis in bilateral hemisphere ROI** | MT | 25 |
| ARMT | 24 |

## 3.1.2 Hand Function Evaluation

SPSS 17.0 was used as a tool for statistical analysis in the experimental results. On the premise that Shapiro-Wilk's test was used to verify that the collected subject data set conforms to the normal distribution, repeated measurement analysis of variance (ANOVA) was used to verify whether there is a significant difference among the three conditions, that is, pre-test, post-test of MT and post-test of ARMT difference. The null hypothesis (H0) before the analysis is that there is no significant difference between these three different conditions, which assumes that no matter whether MT or ARMT intervention is used, there is no short-term improvement in the hand function of healthy subjects from the statistical data. Defined when the p value is less than 0.05, the result is considered to reject the H0. **Table** 7.1shows the outcome measures result in each assessment scale.

**Table** 7.2shows the difference in outcome measures between pre- and post-test in each assessment scale and different conditions for 30 healthy subjects. The focus of the statistical analysis is to compare the pre-test results before intervention as the baseline condition with ARMT condition or MT condition, also insight ARMT's potential well efficacy by comparing the difference is significant between it and MT condition. The chart shows that no matter which intervention method is used, under the indicators of PPT of Dominant hand, PPT of both hands, PPT of assembly, MMDT of placing and MMDT of turning, the intervention of ARMT or MT can make healthy subjects have a short-term and significant differences in these scores. However, the SWM results in this chart also show that neither intervention affected subjects' performance on finger sensation. The following content will graph the results of each hand function assessment tool for more detailed observation.

Table 7.1. The outcome measures in each assessment scale

**\*DH: dominant hand, \*BH: both hands**

|  |  |  |  |
| --- | --- | --- | --- |
| Effectiveness | Baseline (pretest) | ARMT | MT |
| PHUA (FRpeak) | 3.35 ± .64 | 3.01 ± .56 | 3.30 ± .60 |
| PHUA  Percentage (%) | 42.10 ± 13.70 | 34.70 ± 11.00 | 39.00 ± 11.90 |
| PPT (DH) | 14.98 ± 1.69 | 17.20 ± 1.61 | 15.90 ± 1.48 |
| PPT (non-DH) | 14.75 ± 1.34 | 16.02 ± 1.52 | 12.97 ± 1.49 |
| PPT (BH) | 12.48 ± 1.49 | 14.05 ± 1.26 | 13.27 ± 1.09 |
| PPT (Assembly) | 40.43 ± 5.38 | 46.33 ± 5.74 | 42.53 ± 5.63 |
| SWM (Thumb) | 2.39 ± .04 | 2.38 ± .04 | 2.38 ± .04 |
| SWM (Index finger) | 2.36 ± .14 | 2.35 ± .1**4** | 2.36 ± .14 |
| 2PD (Thumb) | 3.40 ± .70 | 3.10 ± .60 | 3.30 ± .60 |
| 2PD (Index finger) | 3.20 ± .50 | 2.60 ± .60 | 3.10 ± .60 |
| MMDT (Placing) | 63.37 ± 6.95 | 58.39 ± 5.93 | 61.39 ± 6.99 |
| MMDT (Turning) | 48.06 ± 5.80 | 41.42 ± 5.12 | 43.81 ± 6.41 |

Table 7.2. P value of pairwise comparison in three conditions

|  |  |  |  |
| --- | --- | --- | --- |
| Effectiveness (*p*) | Baseline vs ARMT | Baseline vs MT | ARMT vs MT |
| PHUA (FRpeak) | .003 | .513 | .002 |
| PHUA  (Force ratio) | < .001 | .105 | .021 |
| PPT (DH) | < .001 | < .001 | < .001 |
| PPT (non-DH) | < .001 | .380 | .001 |
| PPT (BH) | < .001 | .001 | .001 |
| PPT (Assembly) | < .001 | .001 | < .001 |
| SWM (Thumb) | .161 | .662 | .662 |
| SWM (Index finger) | .184 | 1.000 | .264 |
| 2PD (Thumb) | .017 | .601 | .070 |
| 2PD (Index finger) | < .001 | .489 | < .001 |
| MMDT (Placing) | < .001 | .002 | < .001 |
| MMDT (Turning) | < .001 | < .001 | < .001 |

The chart result of PHUA shows in **Figure 33.1**, The intervention of ARMT resulted in a significant reduction in the two evaluation indicators (**FRpeak: *p = .003*, Percentage: *p < .001***), which did not appear in the results of the MT group (**FRpeak: *p = .513*, Percentage: *p = .105***). There are also significant differences between ARMT and MT (**FRpeak: *p = .002*, Percentage: *p = .021***). This phenomenon can be regarded as ARMT has more potential to improve precise control of pinch force than MT to subjects, and the impact of MT's intervention is limited.

Figure 33.1. Chart result of PHUA

**FRpeak result (left), Percentage of maximal pinch strength (right).**

**\**p < .05***

The chart result of PPT shows in **Figure 33.2**, Among four evaluation indicators, MT was significantly different from the baseline in the three (**DH: *p < .001*, BH: *p = .001*, Assembly: *p = .001***), and it is worth mentioning that in the remaining indicator that was not significantly different from the baseline, the score of MT was slightly lower than the baseline (**non-DH:  *Baseline = 14.75, MT = 12.97***). In contrast, the performance of ARMT is better than the baseline and MT conditions, which also have significant differencesin all conditions and evaluation indicators (***p <= .001****)*. This shows that both ARMT and MT interventions can improve the finger dexterity of healthy subjects in the short term. Comparing with MT, ARMT intervention may have a higher potential.

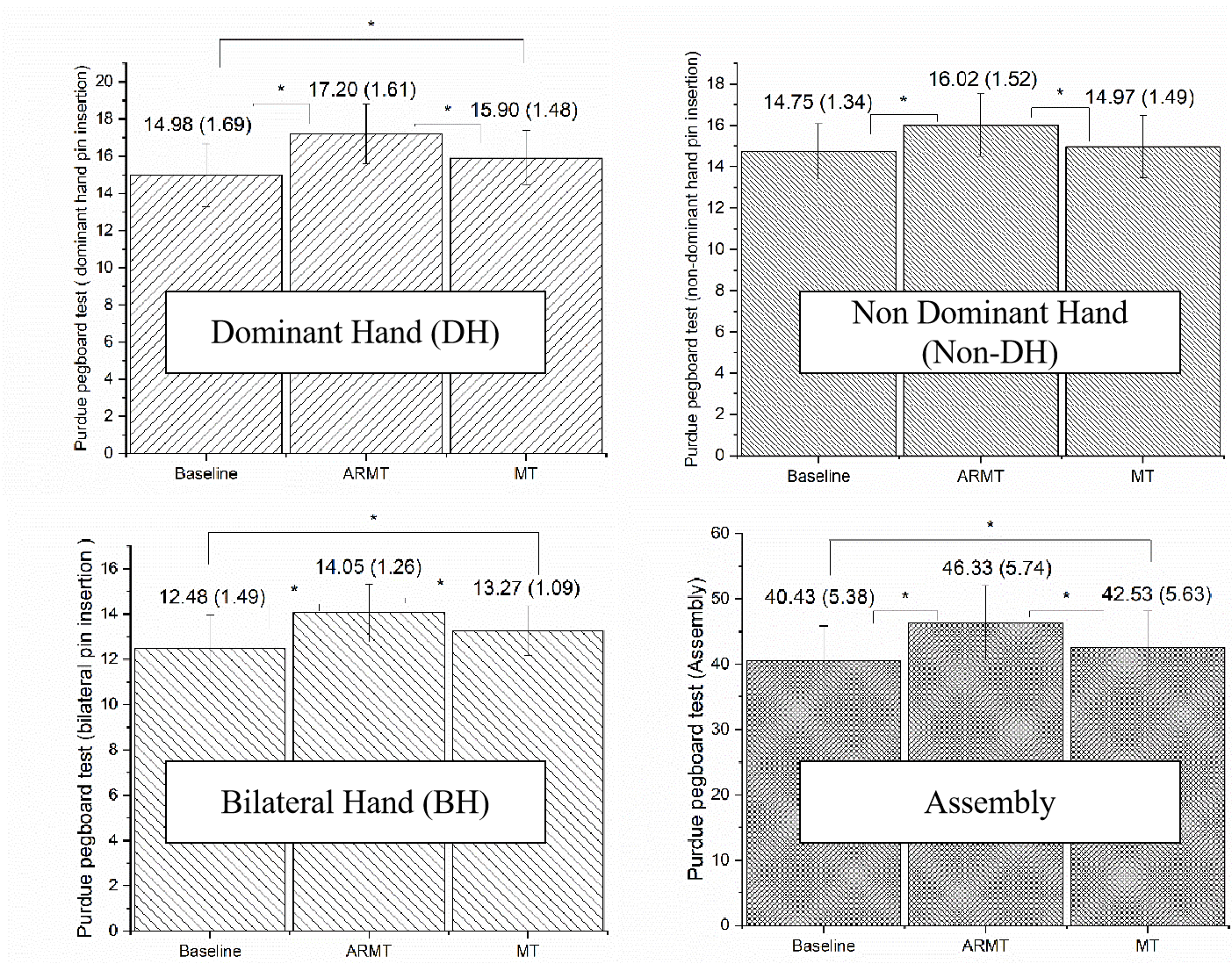


Figure 33.2. Chart result of PPT

**\**p < .05***

No matter the indicator that represents the sensory of the thumb or the index finger, the result of SWM lacks any evidence that any two of the three conditions have a significant difference. However, 2PD test gives two very different results, that is, the two-point distance threshold between the thumb and index finger decreased significantly after ARMT intervention, which means that the subjects can more finely spatial resolution on fingertips, but the intervention of MT has no effect **(Figure 33.3)**.



Figure 33.3. Chart result of 2PD test

**\**p < .05***

The MMDT’s chart result shows in **Figure 33.4**, Among two evaluation indicators, found significant difference in comparison of baseline and MT (**Placing: *p = .002*, Turning: *p < .001***). The condition of Baseline and ARMT has the most significant difference (**Placing: *p < .001*, Turning: *p < .001***), and there is also a high significant difference in the comparison of ARMT and MT conditions (**Placing: *p < .001*, Turning: *p < .001***). This shows that both ARMT and MT interventions can improve the gross motor function of upper extremity of healthy subjects in the short term. Comparing with MT, ARMT intervention may have a higher potential.



Figure 33.4. Chart result of MMDT

**Placing task result (left), turning task result (right).**

**\**p < .05***

## 3.1.3 fNIRS Result of ROI

**Figure 34** shows the fNIRS channels covering the corresponding functional cortex. For channel-wise comparison, the ipsilateral hemisphere of the subject’s moving hand (left hand) will be called the **mirror side** (left hemisphere), while the contralateral hemisphere will be called the **motion side** (right hemisphere). Therefore, in addition to the two intervention methods (ARMT and MT), the channel is divided into four quadrants **(Hemisphere × Cortex Region)** during analysis. Following the 10-block average method estimating blood perfusion trend during the intervention, and the GLM regression method to quantify the activation of cortical areas, several results will describe in figures and tables of the content below.



Figure 34. fNIRS channels covering functional cortex

In the subjects’ prefrontal cortex region, both the MT and the ARMT group observed a tendency towards blood perfusion during the intervention **(Figure 35a, b)**, it takes about 4 to 6 seconds to reach its highest peak after the start of the intervention and then quickly drops below the baseline. For the MT group, the peak of mirror side is slightly behind the motion side. The ARMT group, on the other hand, is almost following the trend of the motion side synchronously. Greater activation of the motion side has been observed no matter in which group. However, the result also reveals a high correlation coefficient of waveform between both sides (**ARMT: *ρ = .961, MT: ρ = .969***).

In the motor cortex region, longer-lasting and more pronounced activation in the motion side was observed in both MT and ARMT group **(Figure 35c, d)**, And the peak of the mirror side in both of the groups are slightly behind than the motion side. Same as the result in prefrontal region, greater activation of the motion side has been observed no matter in which group, but the more the difference (**ARMT: *ρ = .344, MT: ρ = .782***). It is worth mentioning that seems the motion side blood perfusion of ARMT is higher than that of other conditions, therefore, it has a lower correlation coefficient with the ARMT mirror side.

一張含有 文字, 螢幕擷取畫面, 圖表, 行 的圖片

自動產生的描述

Figure 35. Trends in HbO during the intervention

**Prefrontal cortex in ARMT group (a), prefrontal cortex in MT group (b), motor cortex in ARMT group (c) and motor cortex in MT group (d)**

The set of **Table 8.1** shows the beta value result of GLM regression, also applying paired sample t-test to calculate the p value of pairwise comparisons under different conditions to evaluate whether it meets statistically significant differences. Here, the null hypothesis (H0) is defined as the beta value distribution calculated by the two types of conditions should be consistent. If ***p < .05***, it is overturned the hypothesis that there is a statistically significant difference between the two groups of samples.

Result shows the beta value distribution has a very large standard deviation, and there was all no significant difference between the groups (**All conditions: *p > .05***).

Table 8.1. Beta value of fNIRS GLM regression

|  |  |  |  |  |
| --- | --- | --- | --- | --- |
| **Perfusion volume (*β*)** | **ARMT.mirror** | **ARMT.motion** | **MT.mirror** | **MT.motion** |
| **Prefrontal** | 5.02×10-5 ±  1.77×10-4 | 7.13×10-5 ±  1.72×10-4 | 4.54×10-5 ±  1.60×10-4 | 4.59×10-5 ±  1.76×10-4 |
| **Motor** | 3.54×10-5 ±  1.93×10-4 | 4.98×10-5 ±  1.81×10-4 | 5.38×10-5 ±  1.68×10-4 | 3.39×10-5 ±  2.01×10-4 |

Table 8.2. P value in each condition of fNIRS GLM regression

|  |  |  |  |  |  |
| --- | --- | --- | --- | --- | --- |
| **Condition**  **difference (*p)*** | **ARMT**  **(bilateral)** | **MT**  **(bilateral)** | | **Mirror side**  **(ARMT vs MT)** | **Motion side**  **(ARMT vs MT)** |
| **Prefrontal** | .1102 | .9788 | .7977 | | .1827 |
| **Motor** | .1825 | .0842 | .2857 | | .3788 |

The Interquartile range of beta value in ARMT and MT intervention shows in **Figure 36** illustrate the distribution of each condition. In addition to many outliers in the beta value sample, its normal distribution range is relatively wide. In parallel comparison, intuitively, there is little difference under each condition.

一張含有 文字, 圖表, 螢幕擷取畫面, 平行 的圖片

自動產生的描述

Figure 36. Interquartile range of beta value in ARMT and MT intervention

**Prefrontal cortex (a) and motor cortex (b).**

## 3.2 DISCUSSION

Comparing to the MT intervention, several results in the hand function assessment evaluation reveal the more short-term effectiveness in the ARMT intervention may has. Especially the found that the dramatic improvement on finger force coordination in PHUA test and the finger dexterity in subjects’ non-dominant hand in PPT. We attribute this PHUA result to the better immersion of the ARMT and thus possibly better efficacy compared to the MT. For outcomes of non-dominant hand, however, is relatively hard to give a well reason why the ARMT has a better performance, this is because no matter in which types of intervention, the non-dominant hand is always existed truly in the view of subjects’ perspective. As the side actually moving in the intervention, we speculate that the performance of the non-dominant hand should not be significantly different due to any optical illusions.

The same phenomenon also occurred in tactile-related tests. In all the interventions, there was no exercise to improve tactile sensitivity. From the statistical results of SWM, a reasonable conclusion can be drawn, that is, the intervention of MT and ARMT does not make the significantly improved tactile sensitivity. However, in 2PD, there was a contradictory statistical result that the subject's two-point distance threshold decreased significantly after ARMT intervention.

For healthy subjects with normal hand function, proficiency is likely to be the factor affecting the performance of these tests. According to the experimental process designed according to the therapist's clinical experience, for healthy subjects, immediately after the intervention a posterior assessment has a better chance of seeing a significant difference. This may prove that proficiency is a stronger variable. Therefore, the question that needs to be discussed is whether the properties of ARMT can induce healthy subjects to focus more on practicing these repetitive rehabilitation movements? The novelty of the system may be a reason to attract subjects to take the rehabilitation task seriously. Fascinated with the immersive mirror hand image, subjects may have a better willingness to persist on the long-term, boring, repeated rehabilitation task.

For the fNIRS analysis, there may be two reasons for the result of no significant difference: The first point of view is more optimistic, that is, ARMT and MT have similar excitation patterns in these two brain regions of healthy subjects. The second is from the perspective of sample distribution. The differences between samples are too large to analyze. This can be seen from the large standard deviation of beta. However, the large difference may also be related to the signal quality of the received cases. Many subjects encountered great difficulties in data acquiring. Too stiff or thick hair affected the signal quality of fNIRS **(Figure 37)**. These protein structures are easy to block the light source, making it difficult to penetrate the scalp and skull to obtain the trend of HbO in specific superficial cortex.

一張含有 螢幕擷取畫面, 鮮豔, 正方形, 樣式 的圖片

自動產生的描述

Figure 37. The quality of signal acquisition is unstable to each subject

The experimental results also exposed the contradictions in the analysis results between the GLM and the block average method. In terms of the results on the motor cortex, although there is no significant difference in the p value obtained from the GLM regression, it is not the same as the correlation coefficient result, which means that even if the block average perfusion is found similar under the two conditions, but the result of comparing the activation intensity from the perspective of GLM may be different (e.g.: ARMT mirror side vs MT mirror side in motor cortex). The regression model of GLM may not be suitable for every subject, but this may also be related to signal quality.

On the performance of the prefrontal cortex is consistent in the results of the two analysis methods, which slightly endorses the GLM analysis. However, the ARMT motion side is significantly higher than other conditional areas, which does not meet the original assumption of the experimental design. The original assumption was to use the motion side of ARMT and MT as the control group of the mirror side, because we believe that in the same batch of subjects, using MT or ARMT performs the same pinching task, and it will not affect the work of the moving hand. As a result, there will not be much difference in the motion side results of the two interventions. Besides the frequency of pinching, there may be unknown variables in the ARMT intervention that were not controlled in the experiment.

Some literature have found that MT intervention can balance the biased phenomenon of cerebral hemispheres in stroke patients [47, 62], so the ratio of dual-test activation can also be used as a quantitative effect or to evaluate the adaptability of stroke cases to MT. From this point of view, there is a high correlation between ARMT and MT in the blood perfusion pattern of the bilateral prefrontal cortex, but the effect in the bilateral motor sensory cortex is limited, and ARMT may be more lateralized. However, for healthy people, the brain area is not damaged, and the greater lateralization may be general due to the simple relationship between left and right handedness. Therefore, this pilot study cannot directly draw conclusions on the adaptability of ARMT in stroke patients.

The aspect of how ARMT bring convenience to the patient is not evaluated in the research, but the feedback from the subjects after undergoing whole of the intervention mostly guarantee novelty and portability are significantly better than traditional MT or VRMT [4, 5]. Because of the organization and the place that ARMT and VRMT experiment took are the same, also because of the similar outcome measurement and they all use MT as their competitor condition, **Table 9** shows the comparison in between those three different interventions. Although not as direct evidence, it shows that ARMT may have the potential not only to outperform MT, but also in some cases to outperform VRMT.

Table 9. Comparison in between MT, ARMT and VRMT [4]

\*DH: dominant hand, \*BH: both hands

|  |  |  |
| --- | --- | --- |
| Effectiveness (*p*) | MT vs ARMT | MT vs VRMT |
| PHUA (FRpeak) | .002 | .007 |
| PPT (DH) | < .001 | .276 |
| PPT (non-DH) | .001 | .173 |
| PPT (BH) | .001 | .939 |
| PPT (Assembly) | < .001 | .782 |
| MMDT (Placing) | .002 | .490 |
| MMDT (Turning) | < .001 | .544 |

In terms of contributions in the field of stroke rehabilitation, the novelty of ARMT's rendering method surpasses all MT concept software on the Appstore so far [68-70]. Among the existing mobile apps developed with the MT concept, ARMT has the best sense of immersion and screen fluency. The human body semantic segmentation model is a reliable implementation method to optimize the concept of the mirror therapy on mobile devices to provide a better effectiveness **(Figure** 38**)**.

Figure 38. Existing MT Concept Rehabilitation APP [68-70]

一張含有 文字, 螢幕擷取畫面, 人的臉孔 的圖片

自動產生的描述

# Chapter 4 Conclusion and Future Work

## 4.1 CONCLUSION

For the evaluation of hand function, ARMT has a significant effect on short-term gain of most hand functions in healthy subjects compared with MT. Except for perception, both ARMT and MT have found improvement in healthy subjects. The evidence for the conclusion of fNIRS analysis is relatively insufficient, but based on the current analysis, ARMT and MT may have similar excitation patterns in these two brain regions of healthy subjects. As a rehabilitation system positioned between MT and VRMT, ARMT not only has a higher sense of immersion than MT, but also has higher portability and environmental adaptability than VRMT, and novel sensory stimuli have a great chance to attract use the interest and willingness to use of the patient is a part that cannot be ignored in a long-term stroke rehabilitation program.

This study indicates the potential of the ARMT system in the field of rehabilitation at home. Using their personal mobile device, patients in need have an alternative method to traditional MT without requiring additional equipment. The ARMT system can provide a more realistic view that enhances the immersive experience. However, it remains to be seen whether the effectiveness of rehabilitation using ARMT is greater than that of traditional MT, in the purpose of approaching the answer, more clinical stroke trial subjects should be recruited.

## 4.2 LIMITATION

The first limitation of the study is ARMT’s defect, the user must try to avoid other people appearing in the background when using it, otherwise it will cause incorrect rendering of the background portrait to the mirror side. The next limitation is the subject criteria in this pilot study, the healthy subjects included did not have a history of stroke or any brain damage. Therefore, their blood perfusion signal response in the certain cortex may not be representative of the general behavior of stroke patients. Subjects with a history of stroke or hemiplegia will be considered to participate in the experiment in the future.

The possible flaws in the experimental design can also be found from the experimental results. The block average method and the GLM regression method produced inconsistent results, indicating that the experiment may have missed some uncontrolled variables. For example, we found that the specification for the action guidance is not very finely defined in the experiment after performing the clinical trial experiment. In 30 second pinch trial of the block design for fNIRS measurement stage, different subjects have different pinching habits, such as the direction the palm is facing, the force of pinching, and the degree of finger bending. Instead of controlling the frequency of pinching, those differences could be regulated in the future experiment.

Unstable and unpredictable fNIRS signals in between different subjects is another found of experimental flaws. How to obtain the well quality optical signal will be a big challenge for using fNIRS as a benchmark for brain activation quantification. In previous literature survey, some of the researcher utilized EEG for analyzing the intervention influence though the method cannot have spatial resolution comparable to fNIRS, EEG is easier to prepare than fNIRS in the pre-experimental setting and has relatively stable signal quality for different subjects. In terms of results, in this study, we did not effectively use the spatial resolution of fNIRS to achieve a more refined analysis of brain activity. This is because the signal quality among fNIRS channels has not been well set in this study, so the analysis stage can only estimate the activity trend of a specific brain region by averaging a wide range of channels. In this situation, EEG may be a more appropriate choice for pilot experiments that require the collection of large amounts of trend data.

Another flaws in lack of the third control group to handle the condition that the ARMT group result has no significant result comparing to the MT group. Our statistical results cannot confirm whether MT or ARMT has different effects on the brain regions of the subjects than the movement of the one side healthy hand solely, and as evidence that may promote neuroplasticity. Adding a group that signally acquire the fNIRS signal when subjects moving one side of their hand without any kinds of intervention may can be a baseline to evaluate the activation level difference of intervention.

## 4.3 FUTURE WORK

ARMT is still in the development stage, although the results of the pilot experiments are outstanding, the software itself still has potential for optimization. For the future work of optimizing the rendering method, using depth detection to discriminate which texture should be rendered to the mirror side would be one of the directions to solve the current incorrectly render the background portrait defect. On the algorithm of semantic segmentation. Serves as the backbone of the ARMT software, this study introduced the modified Unet and Apple bult-in human segmentation API during the development, several of the model should also be tested in the future, striving to find a more suitable neural network. As the direction of home rehabilitation and telemedicine-type medical equipment, ARMT needs to be able to collect various data from users and send them back to the therapist for reference, and to provide routine or personalized guidance as a way for users to use when the situation without the supervision of the therapist. For this reason, it is a serious and practical direction to develop hand trajectory tracking algorithms on the basis of the existing ones; the second is to try to improve the interaction between the ARMT system and users and improve the compliance and entertainment of patients during rehabilitation, so that it is less likely to feel boring during the rehabilitation process. Designing a task-oriented gameplay reconstruction scheme in the ARMT system can be one of the directions for future development.

## References

[1] B. H. Dobkin, *The clinical science of neurologic rehabilitation*. Oxford University Press, 2003.

[2] R. Teasell *et al.*, “Canadian stroke best practice recommendations: rehabilitation, recovery, and community participation following stroke. Part one: rehabilitation and recovery following stroke; update 2019,” *International Journal of Stroke,* vol. 15, no. 7, pp. 763-788, 2020.

[3] V. S. Ramachandran, D. Rogers-Ramachandran, and S. Cobb, “Touching the phantom limb,” *Nature,* vol. 377, pp. 489-490, 1995.

[4] C.-W. Lin, L.-C. Kuo, Y.-C. Lin, F.-C. Su, Y.-A. Lin, and H.-Y. Hsu, “Development and testing of a virtual reality mirror therapy system for the sensorimotor performance of upper extremity: A pilot randomized controlled trial,” *IEEE Access,* vol. 9, pp. 14725-14734, 2021.

[5] C.-W. Lin, L.-C. Kuo, Y.-C. Lin, F.-C. Su, T.-H. Yang, and H.-Y. Hsu, “Effects of a virtual reality–based mirror therapy program on improving sensorimotor function of hands in chronic stroke patients: a randomized controlled trial,” *Neurorehabilitation and Neural Repair,* vol. 36, no. 6, pp. 335-345, 2022.

[6] (2021). *Global strategy on digital health 2020-2025*.

[7] M. Costandi, *Neuroplasticity*. MIt Press, 2016.

[8] M. Maier, B. R. Ballester, and P. F. Verschure, “Principles of neurorehabilitation after stroke based on motor learning and brain plasticity mechanisms,” *Frontiers in systems neuroscience,* vol. 13, p. 74, 2019.

[9] E. Fuchs and G. Flügge, “Adult neuroplasticity: more than 40 years of research,” *Neural plasticity,* vol. 2014, 2014.

[10] J. Shaffner, “Neuroplasticity and clinical practice: building brain power for health. Front Psychol. 2016; 7: 1118,” ed, 2016.

[11] M. Hallett, “Neuroplasticity and rehabilitation,” *Journal of Rehabilitation Research and Development,* vol. 42, no. 4, p. R17, 2005.

[12] A. Pascual-Leone, “Modulation of motor cortical outputs to the reading hand of braille readers,” *Annals of Neurology,* vol. 34, pp. 33-37, 1993, doi: 10.1002/ana.410340108.

[13] R. J. Nudo, “Functional and structural plasticity in motor cortex: implications for stroke recovery,” *Physical Medicine and Rehabilitation Clinics,* vol. 14, no. 1, pp. S57-S76, 2003.

[14] J. C. Grotta *et al.*, “Constraint-induced movement therapy,” *Stroke,* vol. 35, no. 11\_suppl\_1, pp. 2699-2701, 2004.

[15] M. Hallett, “Plasticity of the human motor cortex and recovery from stroke,” *Brain research reviews,* vol. 36, no. 2-3, pp. 169-174, 2001.

[16] J. Bernhardt, H. Dewey, A. Thrift, and G. Donnan, “Inactive and alone: physical activity within the first 14 days of acute stroke unit care,” *Stroke,* vol. 35, no. 4, pp. 1005-1009, 2004.

[17] J. Livingston-Thomas *et al.*, “Exercise and environmental enrichment as enablers of task-specific neuroplasticity and stroke recovery,” *Neurotherapeutics,* vol. 13, pp. 395-402, 2016.

[18] X. Chen *et al.*, “Therapeutic effects of sensory input training on motor function rehabilitation after stroke,” *Medicine,* vol. 97, no. 48, 2018.

[19] A. Rören, D. M. Yagappa, C. Théry, M.-M. Lefèvre-Colau, F. Rannou, and C. Nguyen, “Remote telerehabilitation to maintain adherence to home-based exercise therapy in people with musculoskeletal disorders: A pilot study,” *Annals of physical and rehabilitation medicine,* vol. 66, no. 5, p. 101723, 2023.

[20] M. White, J. N. Stinson, P. Lingley-Pottie, P. J. McGrath, N. Gill, and A. Vijenthira, “Exploring therapeutic alliance with an internet-based self-management program with brief telephone support for youth with arthritis: a pilot study,” *Telemedicine and e-Health,* vol. 18, no. 4, pp. 271-276, 2012.

[21] M. A. Cottrell, O. A. Galea, S. P. O’Leary, A. J. Hill, and T. G. Russell, “Real-time telerehabilitation for the treatment of musculoskeletal conditions is effective and comparable to standard practice: a systematic review and meta-analysis,” *Clinical rehabilitation,* vol. 31, no. 5, pp. 625-638, 2017.

[22] A. Gover-Chamlou and J. W. Tsao, “Telepain management of phantom limb pain using mirror therapy,” *Telemedicine and e-Health,* vol. 22, no. 2, pp. 176-179, 2016.

[23] T. G. Russell, “Physical rehabilitation using telemedicine,” *Journal of telemedicine and telecare,* vol. 13, no. 5, pp. 217-220, 2007.

[24] T. Hoffmann, T. Russell, L. Thompson, A. Vincent, and M. Nelson, “Using the Internet to assess activities of daily living and hand function in people with Parkinson's disease,” *NeuroRehabilitation,* vol. 23, no. 3, pp. 253-261, 2008.

[25] D. M. Karantonis, M. R. Narayanan, M. Mathie, N. H. Lovell, and B. G. Celler, “Implementation of a real-time human movement classifier using a triaxial accelerometer for ambulatory monitoring,” *IEEE transactions on information technology in biomedicine,* vol. 10, no. 1, pp. 156-167, 2006.

[26] T. Wark, M. Karunanithi, and W. Chan, “A framework for linking gait characteristics of patients with accelerations of the waist,” in *2005 IEEE Engineering in Medicine and Biology 27th Annual Conference*, 2006: IEEE, pp. 7695-7698.

[27] H. M.K, “Virtual environments for motor rehabilitation,” vol. 8, ed: MARY ANN LIEBERT INC 140 HUGUENOT STREET, 3RD FL, NEW ROCHELLE, NY 10801 USA, 2005, pp. 212-212.

[28] K. Laver, S. George, S. Thomas, J. Deutsch, and M. Crotty, “Virtual reality for stroke rehabilitation: an abridged version of a Cochrane review,” *European journal of physical and rehabilitation medicine,* vol. 51, no. 4, pp. 497-506, 2015.

[29] A. Rothgangel and R. Bekrater-Bodmann, “Mirror therapy versus augmented/virtual reality applications: towards a tailored mechanism-based treatment for phantom limb pain,” *Pain management,* vol. 9, no. 2, pp. 151-159, 2019.

[30] R. Kizony, L. Raz, N. Katz, H. Weingarden, and P. L. T. Weiss, “Video-capture virtual reality system for patients with paraplegic spinal cord injury,” *Journal of Rehabilitation Research & Development,* vol. 42, no. 5, 2005.

[31] J. E. Deutsch, A. S. Merians, S. Adamovich, H. Poizner, and G. C. Burdea, “Development and application of virtual reality technology to improve hand use and gait of individuals post-stroke,” *Restorative neurology and neuroscience,* vol. 22, no. 3-5, pp. 371-386, 2004.

[32] M. Park *et al.*, “Effects of virtual reality-based planar motion exercises on upper extremity function, range of motion, and health-related quality of life: a multicenter, single-blinded, randomized, controlled pilot study,” *Journal of neuroengineering and rehabilitation,* vol. 16, no. 1, pp. 1-13, 2019.

[33] R. Miclaus *et al.*, “Non-immersive virtual reality for post-stroke upper extremity rehabilitation: a small cohort randomized trial,” *Brain Sciences,* vol. 10, no. 9, p. 655, 2020.

[34] L. M. Weber, D. M. Nilsen, G. Gillen, J. Yoon, and J. Stein, “Immersive virtual reality mirror therapy for upper limb recovery following stroke: A pilot study,” *American journal of physical medicine & rehabilitation,* vol. 98, no. 9, p. 783, 2019.

[35] K. Marek, I. Zubrycki, and E. Miller, “Immersion Therapy with Head-Mounted Display for Rehabilitation of the Upper Limb after Stroke,” *Sensors,* vol. 22, no. 24, p. 9962, 2022.

[36] S. Hoermann *et al.*, “Computerised mirror therapy with augmented reflection technology for early stroke rehabilitation: clinical feasibility and integration as an adjunct therapy,” *Disability and Rehabilitation,* vol. 39, no. 15, pp. 1503-1514, 2017.

[37] G. A. d. Assis, A. G. D. Corrêa, M. B. R. Martins, W. G. Pedrozo, and R. d. D. Lopes, “An augmented reality system for upper-limb post-stroke motor rehabilitation: a feasibility study,” *Disability and Rehabilitation: Assistive Technology,* vol. 11, no. 6, pp. 521-528, 2016.

[38] A. Boschmann, D. Neuhaus, S. Vogt, C. Kaltschmidt, M. Platzner, and S. Dosen, “Immersive augmented reality system for the training of pattern classification control with a myoelectric prosthesis,” *Journal of neuroengineering and rehabilitation,* vol. 18, no. 1, pp. 1-15, 2021.

[39] C. Zirbel, X. Zhang, and C. Hughes, “The VRehab system: a low-cost mobile virtual reality system for post-stroke upper limb rehabilitation for medically underserved populations,” in *2018 IEEE Global Humanitarian Technology Conference (GHTC)*, 2018: IEEE, pp. 1-8.

[40] T. Labs, “The Evolution of the Myo armband,” ed, 2014.

[41] N. LaPiana *et al.*, “Acceptability of a mobile phone–based augmented reality game for rehabilitation of patients with upper limb deficits from stroke: Case study,” *JMIR rehabilitation and assistive technologies,* vol. 7, no. 2, p. e17822, 2020.

[42] M. Fiala, “Artag, a fiducial marker system using digital techniques, vol. 2,” ed: July, 2005.

[43] Y.-A. Barde, D. Edgar, and H. Thoenen, “Purification of a new neurotrophic factor from mammalian brain,” *The EMBO journal,* vol. 1, no. 5, pp. 549-553, 1982.

[44] E. S. Koroleva *et al.*, “Serum BDNF’s role as a biomarker for motor training in the context of AR-based rehabilitation after ischemic stroke,” *Brain sciences,* vol. 10, no. 9, p. 623, 2020.

[45] M. Ferrari and V. Quaresima, “A brief review on the history of human functional near-infrared spectroscopy (fNIRS) development and fields of application,” *Neuroimage,* vol. 63, no. 2, pp. 921-935, 2012.

[46] J. Mehnert, M. Brunetti, J. Steinbrink, M. Niedeggen, and C. Dohle, “Effect of a mirror-like illusion on activation in the precuneus assessed with functional near-infrared spectroscopy,” *Journal of Biomedical Optics,* vol. 18, no. 6, pp. 066001-066001, 2013.

[47] D. H. Kim, K.-D. Lee, T. C. Bulea, and H.-S. Park, “Increasing motor cortex activation during grasping via novel robotic mirror hand therapy: a pilot fNIRS study,” *Journal of NeuroEngineering and Rehabilitation,* vol. 19, no. 1, pp. 1-14, 2022.

[48] J. J. Zhang, K. N. Fong, N. Welage, and K. P. Liu, “The activation of the mirror neuron system during action observation and action execution with mirror visual feedback in stroke: a systematic review,” *Neural plasticity,* vol. 2018, 2018.

[49] F. G. S. Velez *et al.*, “Real-time video projection in an mri for characterization of neural correlates associated with mirror therapy for phantom limb pain,” *JoVE (Journal of Visualized Experiments),* no. 146, p. e58800, 2019.

[50] C. Neiger. “Virtual reality is too expensive for most people — but that's about to change.” <https://www.businessinsider.com/why-is-virtual-reality-so-expensive-2016-9> (accessed.

[51] “Omdia research reveals 12.5m consumer VR headsets sold in 2021 with content spend exceeding $2bn.” OMDIA. <https://omdia.tech.informa.com/pr/2021-dec/omdia-research-reveals-12m-consumer-vr-headsets-sold-in-2021-with-content-spend-exceeding-2bn> (accessed.

[52] *AVDepthData*. Apple Developer. [Online]. Available: <https://developer.apple.com/documentation/avfoundation/avdepthdata>

[53] Y. Guo, Y. Liu, T. Georgiou, and M. S. Lew, “A review of semantic segmentation using deep neural networks,” *International journal of multimedia information retrieval,* vol. 7, pp. 87-93, 2018.

[54] Z. Qu and L. Zhang, “Research on image segmentation based on the improved Otsu algorithm,” in *2010 Second International Conference on Intelligent Human-Machine Systems and Cybernetics*, 2010, vol. 2: IEEE, pp. 228-231.

[55] A. Dos Anjos and H. R. Shahbazkia, “Bi-level image thresholding,” *Biosignals,* vol. 2, pp. 70-76, 2008.

[56] A. Betancourt, “EgoHands: a unified framework for hand-based methods in first person vision videos,” 2017.

[57] O. Ronneberger, P. Fischer, and T. Brox, “U-net: Convolutional networks for biomedical image segmentation,” in *Medical Image Computing and Computer-Assisted Intervention–MICCAI 2015: 18th International Conference, Munich, Germany, October 5-9, 2015, Proceedings, Part III 18*, 2015: Springer, pp. 234-241.

[58] M. Sandler, A. Howard, M. Zhu, A. Zhmoginov, and L.-C. Chen, “Mobilenetv2: Inverted residuals and linear bottlenecks,” in *Proceedings of the IEEE conference on computer vision and pattern recognition*, 2018, pp. 4510-4520.

[59] L.-C. Chen, G. Papandreou, F. Schroff, and H. Adam, “Rethinking atrous convolution for semantic image segmentation,” *arXiv preprint arXiv:1706.05587,* 2017.

[60] “Core ML Models.” APPLE Developer. <https://developer.apple.com/machine-learning/models/> (accessed.

[61] P. Turner, “ARHeadsetKit: Bringing Affordable AR Headset Technology to the Masses,” Ocean Lakes High School, 2022.

[62] M. Mihara *et al.*, “Cortical control of postural balance in patients with hemiplegic stroke,” *Neuroreport,* vol. 23, no. 5, pp. 314-319, 2012.

[63] S. B. Moro *et al.*, “A semi-immersive virtual reality incremental swing balance task activates prefrontal cortex: a functional near-infrared spectroscopy study,” *Neuroimage,* vol. 85, pp. 451-460, 2014.

[64] J. R. Flanagan and A. M. Wing, “Modulation of grip force with load force during point-to-point arm movements,” *Experimental brain research,* vol. 95, pp. 131-131, 1993.

[65] T. J. Huppert, S. G. Diamond, M. A. Franceschini, and D. A. Boas, “HomER: a review of time-series analysis methods for near-infrared spectroscopy of the brain,” *Applied optics,* vol. 48, no. 10, pp. D280-D298, 2009.

[66] A. von Lühmann, A. Ortega-Martinez, D. A. Boas, and M. A. Yücel, “Using the general linear model to improve performance in fNIRS single trial analysis and classification: a perspective,” *Frontiers in human neuroscience,* vol. 14, p. 30, 2020.

[67] A. von Lühmann, X. Li, K.-R. Müller, D. A. Boas, and M. A. Yücel, “Improved physiological noise regression in fNIRS: a multimodal extension of the general linear model using temporally embedded canonical correlation analysis,” *NeuroImage,* vol. 208, p. 116472, 2020.

[68] T. Kawakami. “MirrorBox Lite.” <https://reurl.cc/p64Dl8> (accessed.

[69] A. GmbH. “AS-Mirror.” <https://reurl.cc/mD4nLj> (accessed.

[70] S. R. P. T. P.A. “Mirror Box: CRPS & RSD, Stroke.” <https://reurl.cc/VLQ68Y> (accessed.

1. \* 研究生 [↑](#footnote-ref-1)
2. \*\* 指導教授 [↑](#footnote-ref-2)
3. \* Student [↑](#footnote-ref-3)
4. \*\* Advisor [↑](#footnote-ref-4)