

An ALE Finite Element Method for Vorticity-Streamfunction Formulation with Species Transport Equation

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Outline

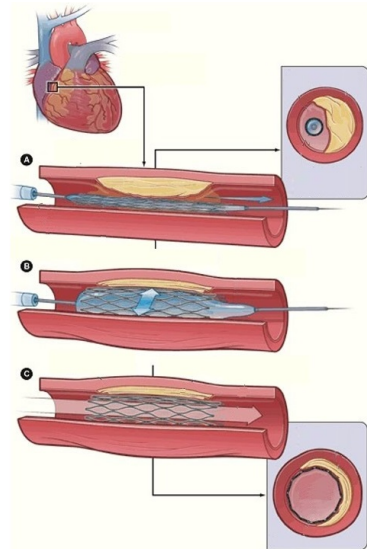
1. Introduction
2. Mathematical Model
3. Computational Code
4. Validation
5. Results
6. Conclusion

Motivation:

- Ischaemic heart disease and stroke have remained the leading death causes globally in the last 15 years [1]

Goals:

- To develop a ALE-FE code for the Vorticity-Streamfunction Formulation
- To create new drug-eluting stent design patent



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Arbitrary Lagrangian-Eulerian (ALE)

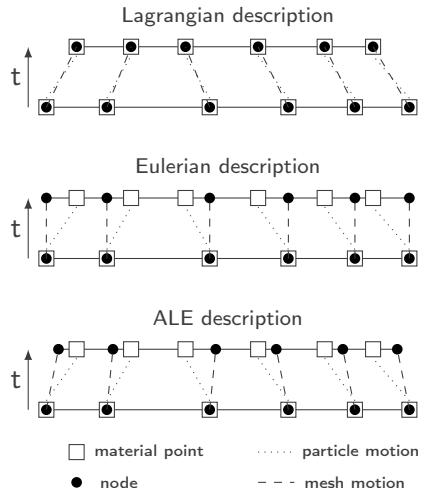
The Arbitrary Lagrangian-Eulerian combines the classical motion descriptions, while it provides [2]:

Advantages:

- Simulations in fluid-structure and moving boundary problems

Disadvantages:

- The computational mesh requires an extensive topological treatment



[2] Donea, J., Huerta, A., Ponthot, J.-P. and Rodríguez-Ferran, A. (2004). Arbitrary Lagrangian-Eulerian Methods. In Encyclopedia of Computational Mechanics *doi:10.1002/0470091355.ecm009*

Governing Equations

Assumptions [3]:

1. Continuum hypothesis
2. Homogeneous and Isotropic
3. Incompressible
4. Newtonian
5. Constant Mass Difusivity
6. Single-phase Flow
7. Two-dimensional flow

$$\frac{\partial \omega}{\partial t} + (\mathbf{v} - \hat{\mathbf{v}}) \cdot \nabla \omega = \frac{1}{Re} \nabla^2 \omega$$

$$\nabla^2 \psi = -\omega$$

$$\frac{\partial e}{\partial t} + (\mathbf{v} - \hat{\mathbf{v}}) \cdot \nabla e = \frac{1}{ReSc} \nabla^2 e$$

- If the mesh velocity field $\hat{\mathbf{v}} = \mathbf{v}$ (*Lagrangian*) or $\hat{\mathbf{v}} = 0$ (*Eulerian*)
- The material velocity field $\mathbf{v} = (v_x, v_y)$ is calculated by:
 $v_x = \partial \psi / \partial y$ and $v_y = -\partial \psi / \partial x$

Semi-Lagrangian Method

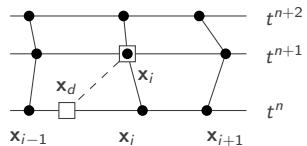
The convective term was replaced by material derivative in the direction of characteristic trajectory, that is: $\frac{D(\cdot)}{Dt} = \frac{\partial(\cdot)}{\partial t} + (\mathbf{v} - \hat{\mathbf{v}}) \cdot \nabla(\cdot)$

$$\frac{D\omega}{Dt} = \frac{1}{Re} \nabla^2 \omega$$

$$\nabla^2 \psi = -\omega$$

$$\frac{De}{Dt} = \frac{1}{ReSc} \nabla^2 e$$

The departure node is calculated by $x_d^n = x_i^{n+1} - (\mathbf{v} - \hat{\mathbf{v}}) \Delta t$. Then, a searching procedure is required to find x_d^n using barycentric coordinates



The implicit semi-Lagrangian time discretization provides [4]:

Advantages:

- ▶ Symmetric linear systems
- ▶ Unconditionnal stability

$$\frac{\omega_i^{n+1} - \omega_d^n}{\Delta t} = \frac{1}{Re} \nabla^2 \omega^{n+1}$$

$$\nabla^2 \psi = -\omega$$

Disadvantages:

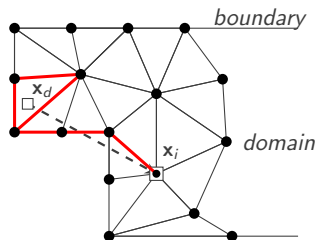
- ▶ Numerical Diffusion
- ▶ Searching procedure may lead to excessive computational cost if it is not well designed

$$\frac{e_i^{n+1} - e_d^n}{\Delta t} = \frac{1}{ReSc} \nabla^2 e^{n+1}$$

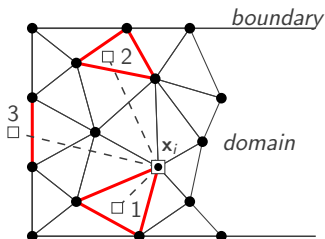
[4] Pironneau, O. On the transport-diffusion algorithm and its applications to the Navier-Stokes equations. Numer. Math. 38, 309–332 (1982). <https://doi.org/10.1007/BF01396435>

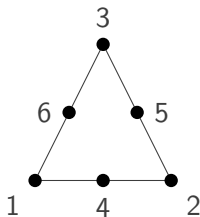
Searching Procedure

The convective term was replaced by material derivative in the direction of characteristic trajectory, that is: $\frac{D(\cdot)}{Dt} = \frac{\partial(\cdot)}{\partial t} + (\mathbf{v} - \hat{\mathbf{v}}) \cdot \nabla(\cdot)$

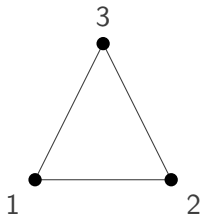


The departure node is calculated by $x_d^n = x_i^{n+1} - (\mathbf{v} - \hat{\mathbf{v}}) \Delta t$. Then, a searching procedure is required to find x_d^n using barycentric coordinates





Quad Element



Linear Element

$$\left[\frac{\mathbf{M}}{\Delta t} + \frac{\mathbf{K}}{Re} \right] \omega_i^{n+1} = \frac{\mathbf{M}}{\Delta t} \omega_d^n$$

$$\mathbf{K}\psi = \mathbf{M}\omega$$

$$\left[\frac{\mathbf{M}}{\Delta t} + \frac{\mathbf{K}}{ReSc} \right] e_i^{n+1} = \frac{\mathbf{M}}{\Delta t} e_d^n$$

- The material velocity field is calculated by:

$$\mathbf{M}v_x = \mathbf{G}_y\psi$$

$$\mathbf{M}v_y = -\mathbf{G}_x\psi$$

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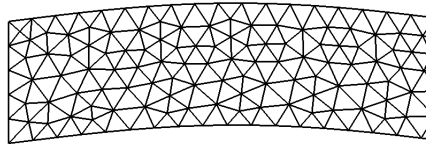
Laplacian Smoothing

To avoid the fast degradation of the computational elements due to ALE description, it was used the Laplacian Smoothing Method [5]

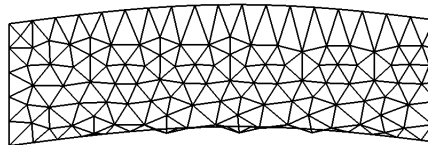
The new node position \hat{x}_i can be approximated by:

$$\hat{x}_i = w_{ij} \sum_j^{N_1} (x_j - x_i)$$

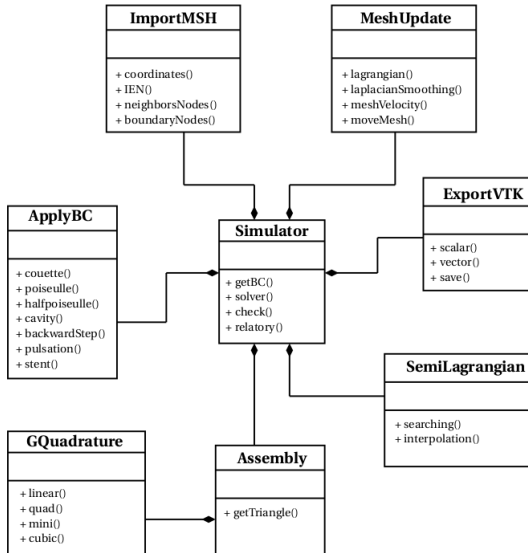
where, N_1 is the 1-ring neighbors of the node, w_{ij} is the weight and was calculated by the inverse distance from neighbors vertices



with Laplacian Smoothing



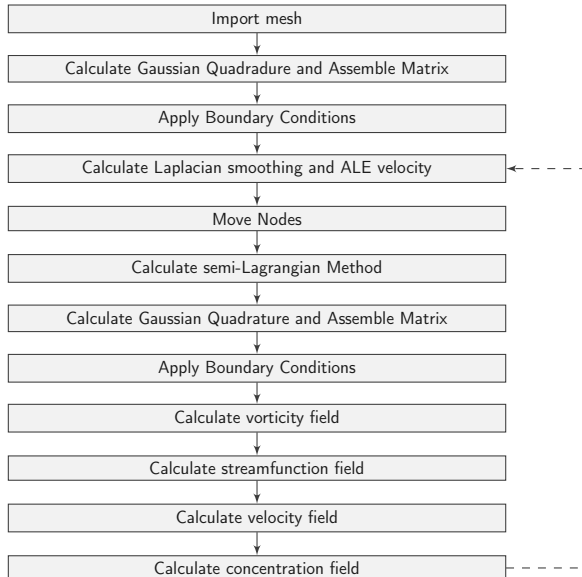
no Laplacian Smoothing



Process	AVG Computational Cost (%)
Mesh import	1.24
Assembly	73.87
BC Apply	6.70
Mesh update	10.05
Semi-Lagrangian	2.27
Vorticity Solver	5.51
VTK export	0.36

Average computational cost for the linear triangular element.

Solution Algorithm



Repeat the procedure
for the next time step
until the steady state

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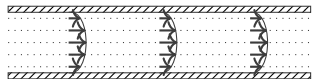
Validation - Poiseuille Flow

Boundaries Conditions:

Inflow condition: $u = u_{analytical}$, $v = 0$

Top plate: $u = 0$, $v = 0$, $\psi = 1$

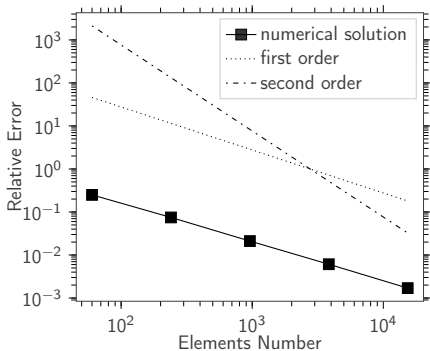
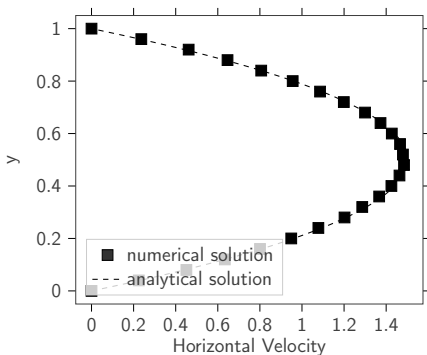
Bottom plate: $u = 0$, $v = 0$, $\psi = 0$



Nodes: 1757

Elements: 3263

Relative Error: 1.2%



Validation - Lid Driven Cavity Flow

Boundaries Conditions:

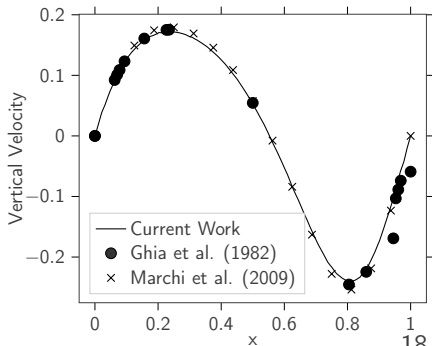
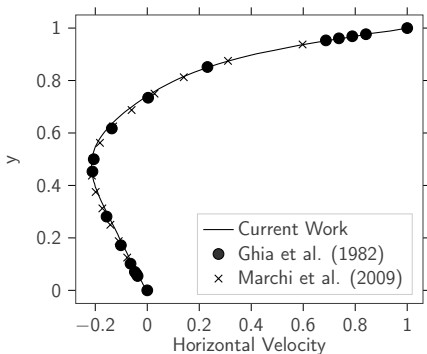
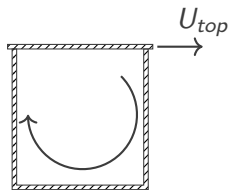
Bottom and side plates: $u = 0$, $v = 0$ e $\psi = 0$

Top plate: $u = 1$, $v = 0$ e $\psi = 0$

Nodes: 3798

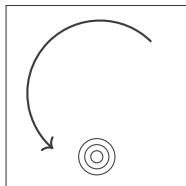
Elements: 7382

Re: 100



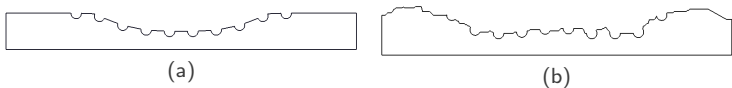
Hipóteses:

1. Fluido como um Meio Contínuo
2. Fluido incompressível
3. Fluido newtoniano
4. Escoamento monofásico
5. Escoamento bidimensional
6. Elevado número de Reynolds ($Re = \infty$)



$$\frac{\partial c}{\partial t} + \mathbf{v} \cdot \nabla c = 0$$

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Non-dimensional symmetric geometry for blood flow in coronary artery with drug-eluting stent placed by Wang et al. (2017): (a) Curved Channel with Stent (b) Real Channel with Stent.

Boundaries Conditions:

Inflow condition: $u = 1$, $v = 0$ e $\psi = y$;

Outflow condition: $\psi = y$;

Top plate: $u = 0$, $v = 0$, $\psi = 1$;

Symmetry condition: $v = 0$, $\psi = 0$;

Drug-eluting stent: $u = 0$, $v = 0$, $\psi = 1$ e $c = 1$

$$R = 0.0015m$$

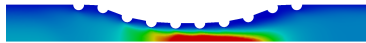
$$\mu = 0.0035Pa.s$$

$$\rho = 1060kg/m^3$$

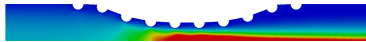
$$u = 12cm/s$$

$$Re = 54.5$$

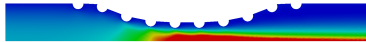
Results - Velocity Field



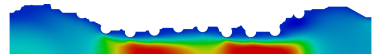
$t = 1.0$



$t = 5.0$



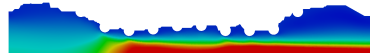
$t = 10.0$



$t = 1.0$

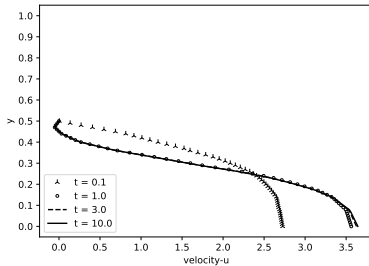


$t = 5.0$

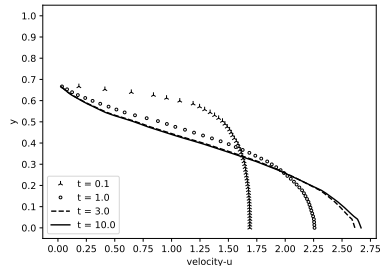


$t = 10.0$

Evolution in time and space of velocity field:
Curved Channel (left column) and Real Channel (right column)



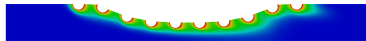
(a)



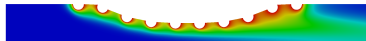
(b)

Evolution of velocity profile in centerline ($x = 0.5L$):
(a) Curved Channel and (b) Real Channel

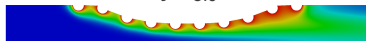
Results - Concentration Field



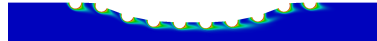
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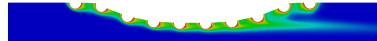
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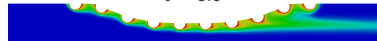
$t = 10.0$



$t = 1.0$

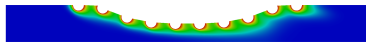


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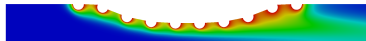


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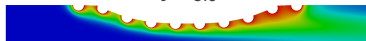
Evolution in time and space of concentration field in Curved Channel:
 $Sc = 1$ (left column) and $Sc = 10$ (right column)



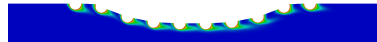
$t = 1.0$



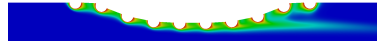
$t = 5.0$



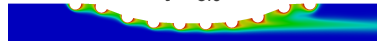
$t = 10.0$



$t = 1.0$



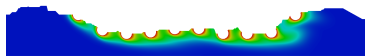
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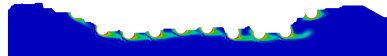
$t = 10.0$

Evolution in time and space of concentration field in Real Channel:
 $Sc = 1$ (left column) and $Sc = 10$ (right column)

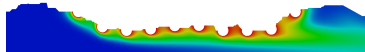
Results - Concentration Field



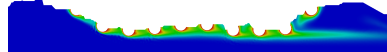
$t = 1.0$



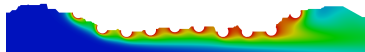
$t = 1.0$



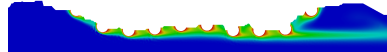
$t = 5.0$



$t = 5.0$

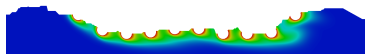


$t = 10.0$

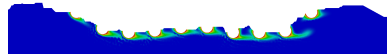


$t = 10.0$

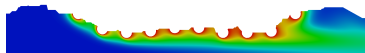
Evolution in time and space of concentration field in Curved Channel:
 $Sc = 1$ (left column) and $Sc = 10$ (right column)



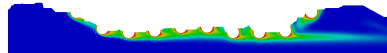
$t = 1.0$



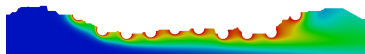
$t = 1.0$



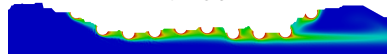
$t = 5.0$



$t = 5.0$



$t = 10.0$



$t = 10.0$

Evolution in time and space of concentration field in Real Channel:
 $Sc = 1$ (left column) and $Sc = 10$ (right column)

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1. The streamfunction-vorticity formulation showed an useful approach for to calculate the velocity and concentration fields since the variables are scalars allowing a smooth implementation
2. Due to generalized construction of the code, the simulator is able to describe drug-eluting stent problem in coronary artery as well as flows of Newtonian fluids with scalar transport (concentration or temperature)
3. The ALE description allows moving boundary problems to be simulated

Thank you!

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