A ALE Finite Element Method for Vorticity-Streamfunction Formulation with Species Transport Equation

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Outline



- 1. Introduction
- 2. Mathematical Model
- 3. Validation
- 4. Results
- 5. Conclusion

Introduction

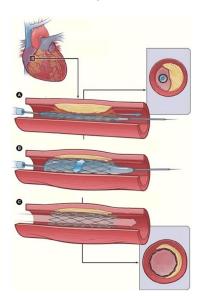


Motivation:

► Ischaemic heart disease and stroke have remained the leading death causes globally in the last 15 years [1]

Aims:

- ► To develop a Finite Element code for stream-vorticity formulation with species transport equation using the Arbitrary Lagrangian-Eulerian (ALE) approach
- ► To create new drug-eluting design patent





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Arbitrary Lagrangian-Eulerian (ALE)



The Arbitrary Lagrangian-Eulerian combines the classical motion descriptions, while it provides [2]:

Lagrangian description

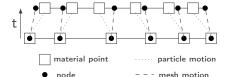
Advantages:

► Simulations in fluid-structure and moving boundary problems

Eulerian description

Disadvantages:

► The computational mesh requires an extensive topological treatment



node

ALE description

[2] Donea, J., Huerta, A., Ponthot, J.-P. and Rodríguez-Ferran, A. (2004). Arbitrary Lagrangian–Eulerian Methods. In Encyclopedia of Computational Mechanics doi:10.1002/0470091355.ecm009

Governing Equations



Assumptions [3]:

- 1. Continuum hypothesis
 - 2. Homogeneous and Isotropic
 - 3. Incompressible
 - 4. Newtonian
 - 5. Constant Mass Difusivity
 - 6. Single-phase Flow
 - 7. Two-dimensional flow

$$\frac{D\omega}{Dt} = \frac{1}{Re} \nabla^2 \omega$$

$$\nabla^2 \psi = -\omega$$

$$\frac{Dc}{Dt} = \frac{1}{ReSc} \nabla^2 c$$

where, $D(\cdot)/Dt$ is substantive derivative and the material velocity field is calculated by: $v_x = \partial \psi/\partial y$ and $v_y = -\partial \psi/\partial x$

Semi-Lagrangian Method



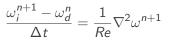
The implicit semi-Lagrangian time discretization provides [4]:

Advantages:

- ► Symmetric linear systems
- ► Unconditionnal stability

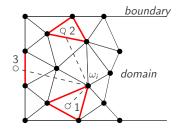
Disadvantages:

- ► Numerical Diffusion
- Searching procedure may lead to excessive computational cost if it is not well designed



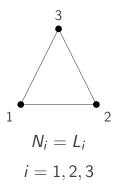
$$\nabla^2 \psi = -\omega$$

$$\frac{c_i^{n+1} - c_d^n}{\Delta t} = \frac{1}{ReSc} \nabla^2 c^{n+1}$$



Galerkin FE Method





$$\begin{bmatrix} \frac{\mathsf{M}}{\Delta t} + \frac{\mathsf{K}}{Re} \end{bmatrix} \omega_i^{n+1} = \frac{\mathsf{M}}{\Delta t} \omega_d^n$$

$$\mathsf{K} \psi = \mathsf{M} \omega$$

$$\left[\frac{\mathsf{M}}{\Delta t} + \frac{\mathsf{K}}{\mathsf{ReSc}}\right] c_i^{n+1} = \frac{\mathsf{M}}{\Delta t} c_d^n$$

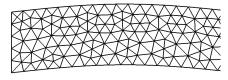
The material velocity field is calculated by: $\mathbf{M} v_{\mathbf{x}} = \mathbf{G}_{\mathbf{y}} \psi$ and $\mathbf{M} v_{\mathbf{y}} = -\mathbf{G}_{\mathbf{x}} \psi$

Mesh Smoothing



Motivation:

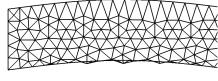
► Ischaemic heart disease and stroke have remained the leading death causes globally in the last 15 years [1]



with ALE

Aims:

► To develop a Finite Element code for stream-vorticity formulation with species transport equation using the Arbitrary Lagrangian-Eulerian

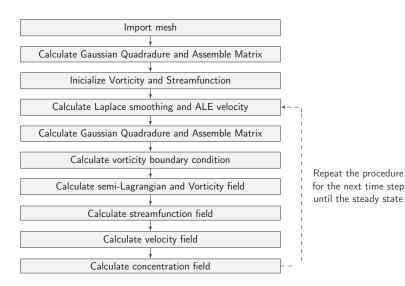


without ALE

- (ALE) approach [1] World Health Organization, 2018, "The top 10 causes of death". www.who.int/news-room/fact-sheets/detail/the-top-10-causes-of-death [Online accessed 06-04-20 08:27pm]
- ► To create new drug-eluting design patent

Solution Algorithm







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Validation - Poiseuille Flow



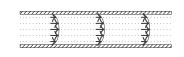
Boundaries Conditions:

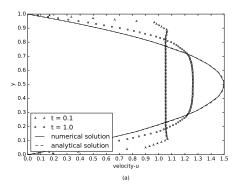
Inflow condition: u = 1, v = 0 e $\psi = y$

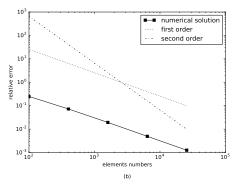
Outflow condition: $\psi = y$

Top plate: u= 0, v= 0, $\psi=$ 1

Bottom plate: u= 0, v= 0, $\psi=$ 0







(a) comparison of Poiseuille Flow velocity profile and (b) log scale graph of convergence order.

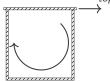
Validation - Lid Driven Cavity Flow

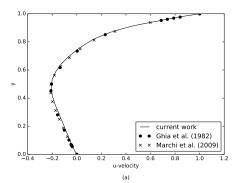


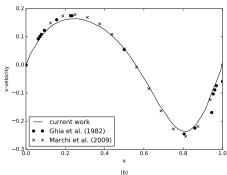
Boundaries Conditions:

Bottom and side plates: $\it u=0$, $\it v=0$ e $\it \psi=0$

Top plate: u=1, v=0 e $\psi=0$







Centerline velocity profile in a lid-driven cavity for Re = 100: (a) u-velocity and (b) v-velocity.





Coming Soon

Validation - Pulsation Flow



Coming Soon



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Results



Coming Soon



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Conclusion



- 1. Was observed that the species transport in blood flow is directly influenced by drug used in stent production
- 2. The streamfunction-vorticity formulation showed an useful approach for to calculate the velocity and concentration fields since the variables are scalars allowing a smooth implementation
- 3. Due to generalized construction of the code, the simulator is able to describe drug-eluting stent problem in coronary artery as well as flows of Newtonian fluids with scalar transport (concentration or temperature)



Thank you!

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