

# An ALE Finite Element Method for Vorticity-Streamfunction Formulation with Species Transport Equation

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# Outline

1. Introduction
2. Mathematical Model
3. Validation
4. Results
5. Conclusion

# Introduction

## Motivation:

- Ischaemic heart disease and stroke have remained the leading death causes globally in the last 15 years [1]

## Aims:

- To develop a Finite Element code for stream-vorticity formulation with species transport equation using the Arbitrary Lagrangian-Eulerian (ALE) approach
- To create new drug-eluting stent design patent



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# Arbitrary Lagrangian-Eulerian (ALE)

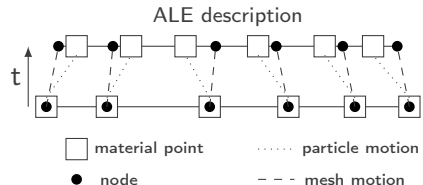
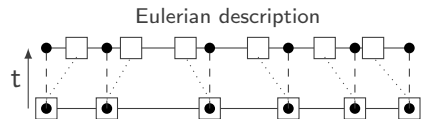
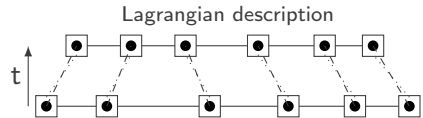
The Arbitrary Lagrangian-Eulerian combines the classical motion descriptions, while it provides [2]:

Advantages:

- Simulations in fluid-structure and moving boundary problems

Disadvantages:

- The computational mesh requires an extensive topological treatment



[2] Donea, J., Huerta, A., Ponthot, J.-P. and Rodríguez-Ferran, A. (2004). Arbitrary Lagrangian-Eulerian Methods. In Encyclopedia of Computational Mechanics *doi:10.1002/0470091355.ecm009*

# Governing Equations

Assumptions [3]:

1. Continuum hypothesis
2. Homogeneous and Isotropic
3. Incompressible
4. Newtonian
5. Constant Mass Difusivity
6. Single-phase Flow
7. Two-dimensional flow

$$\frac{\partial \omega}{\partial t} + (\mathbf{v} - \hat{\mathbf{v}}) \cdot \nabla \omega = \frac{1}{Re} \nabla^2 \omega$$

$$\nabla^2 \psi = -\omega$$

$$\frac{\partial c}{\partial t} + (\mathbf{v} - \hat{\mathbf{v}}) \cdot \nabla c = \frac{1}{ReSc} \nabla^2 c$$

- If the mesh velocity field  $\hat{\mathbf{v}} = \mathbf{v}$  (*Lagrangian*) or  $\hat{\mathbf{v}} = 0$  (*Eulerian*)
- The material velocity field  $\mathbf{v} = (v_x, v_y)$  is calculated by:  
 $v_x = \partial \psi / \partial y$  and  $v_y = -\partial \psi / \partial x$

# Semi-Lagrangian Method

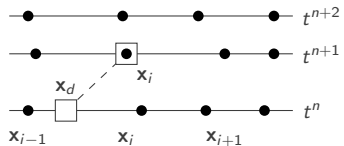
The convective term was replaced by material derivative in the direction of characteristic trajectory, that is:  $\frac{D(\cdot)}{Dt} = \frac{\partial(\cdot)}{\partial t} + (\mathbf{v} - \hat{\mathbf{v}}) \cdot \nabla(\cdot)$

$$\frac{D\omega}{Dt} = \frac{1}{Re} \nabla^2 \omega$$

$$\nabla^2 \psi = -\omega$$

$$\frac{Dc}{Dt} = \frac{1}{ReSc} \nabla^2 c$$

The departure node is calculated by  $x_d^n = x_i^{n+1} - (\mathbf{v} - \hat{\mathbf{v}}) \Delta t$ . Then, a searching procedure is required to find  $x_d^n$  using barycentric coordinates



# Semi-Lagrangian Method

The implicit semi-Lagrangian time discretization provides [4]:

Advantages:

- Symmetric linear systems
- Unconditionnal stability

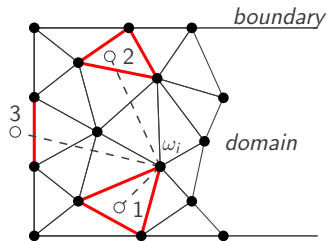
Disadvantages:

- Numerical Diffusion
- Searching procedure may lead to excessive computational cost if it is not well designed

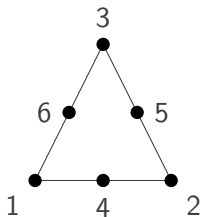
$$\frac{\omega_i^{n+1} - \omega_d^n}{\Delta t} = \frac{1}{Re} \nabla^2 \omega^{n+1}$$

$$\nabla^2 \psi = -\omega$$

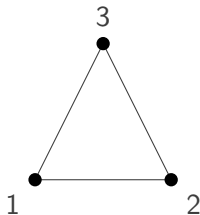
$$\frac{c_i^{n+1} - c_d^n}{\Delta t} = \frac{1}{ReSc} \nabla^2 c^{n+1}$$







Quad Element



Linear Element

$$\left[ \frac{\mathbf{M}}{\Delta t} + \frac{\mathbf{K}}{Re} \right] \omega_i^{n+1} = \frac{\mathbf{M}}{\Delta t} \omega_d^n$$

$$\mathbf{K}\psi = \mathbf{M}\omega$$

$$\left[ \frac{\mathbf{M}}{\Delta t} + \frac{\mathbf{K}}{ReSc} \right] c_i^{n+1} = \frac{\mathbf{M}}{\Delta t} c_d^n$$

- The material velocity field is calculated by:

$$\mathbf{M}v_x = \mathbf{G}_y\psi$$

$$\mathbf{M}v_y = -\mathbf{G}_x\psi$$

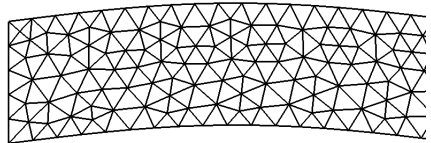
# Laplacian Smoothing

To avoid the fast degradation of the computational elements due to ALE description, it was used the Laplacian Smoothing Method [5]

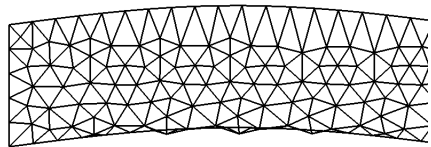
The new node position  $\hat{\mathbf{x}}_i$  can be approximated by:

$$\hat{\mathbf{x}}_i = \sum_{i \in N_1} e_{ij}^{-1} (\mathbf{x}_j - \mathbf{x}_i)$$

where,  $e_{ij}^{-1}$  is the distance between the node and each neighbor in 1-ring  $N_1$



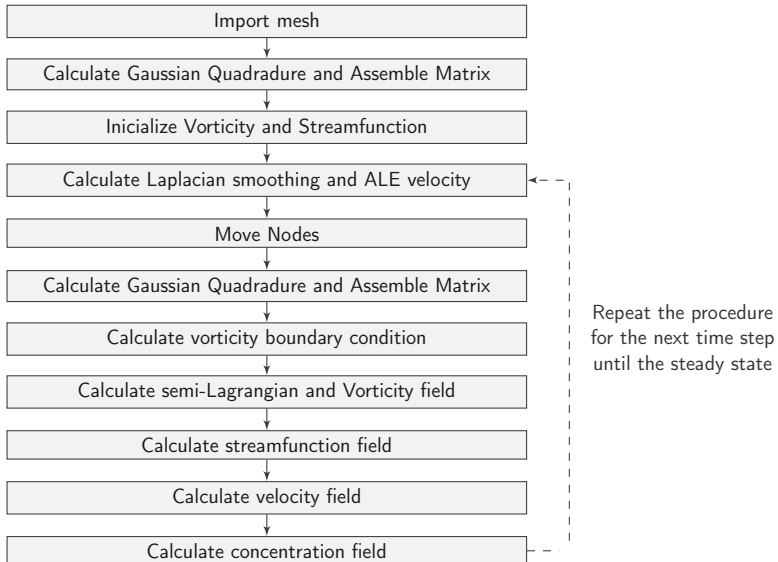
with Laplacian Smoothing



no Laplacian Smoothing

[5] Desbrun, M. Meyer, P. Schröder, A. Barr, Implicit fairing of irregular meshes using diffusion and curvature flow, in: Proceedings of Siggraph, 1999, pp. 317–324

# Solution Algorithm



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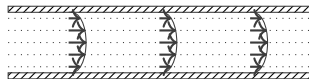
# Validation - Poiseuille Flow

Boundaries Conditions:

Inflow condition:  $u = u_{analytical}$ ,  $v = 0$

Top plate:  $u = 0$ ,  $v = 0$ ,  $\psi = 1$

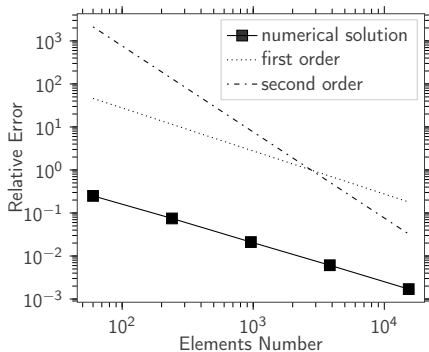
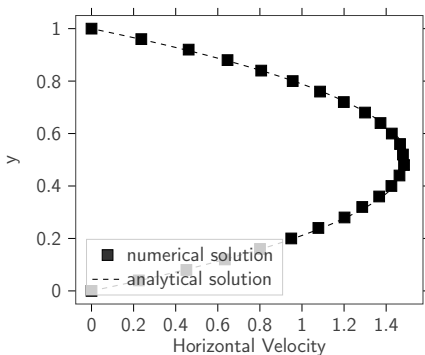
Bottom plate:  $u = 0$ ,  $v = 0$ ,  $\psi = 0$



Nodes: 1757

Elements: 3263

Relative Error: 1.2%



# Validation - Lid Driven Cavity Flow

Boundaries Conditions:

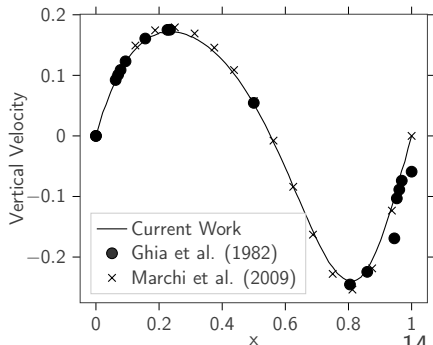
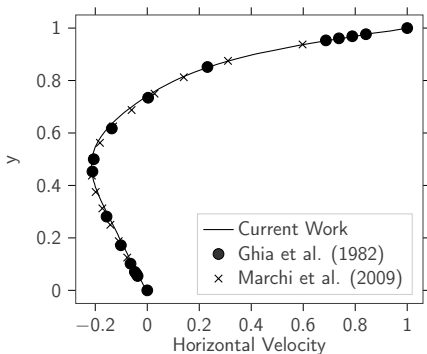
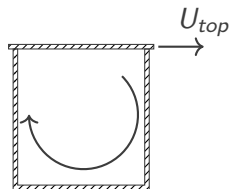
Bottom and side plates:  $u = 0$ ,  $v = 0$  e  $\psi = 0$

Top plate:  $u = 1$ ,  $v = 0$  e  $\psi = 0$

Nodes: 3798

Elements: 7382

Re: 100



# Coming Soon

- ▶ Backward-Facing Step Validation
- ▶ Pulsation Flow Validation
- ▶ Drug-Eluting Stent Cases

# Work Plan

	2018				2019								2020												
ACTIVITIES	9	10	11	12	1	2	3	4	5	6	7	8	9	10	11	12	1	2	3	4	5	6	7	8	
SUBJECTS																									
LITERATURE REVIEW																									
CODE IMPLEMENTATION																									
CODE VALIDATION																									
RESULTS SIMULATION																									
PRESENTATION																									

## SUBJECTS:

- CONTINUUM MECHANICS I
- ADVANCED CALCULUS
- FLUID MECHANICS
- COMPUTATIONAL FLUID MECHANICS I
- COMPUTATIONAL FLUID MECHANICS II
- FINITE ELEMENT METHOD
- COMPUTATIONAL METHODS
- MULTIPHASE FLOWS

## LITERATURE REVIEW:

- ARBITRARY LAGRANGIAN-EULERIAN (ALE)
- SEMI-LAGRANGIAN METHOD
- LAPLACIAN SMOOTHING



## Expected Date for Final Presentation

August 2020      < >

	S	M	T	W	T	F	S
31	26	27	28	29	30	31	1
32	2	3	4	5	6	7	8
33	9	10	11	12	13	14	15
34	16	17	18	19	20	21	22
35	23	24	25	26	27	28	29
36	30	31	1	2	3	4	5

# Thank you!

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