



Statistical methods for wearable device data and sample size calculation in complex models

Marta Karas

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Recording from the defense presentation:

<https://youtu.be/xST4dqInxBo>

About

Profile

- 5th year PhD candidate in Biostatistics at Johns Hopkins University
 - Wearable and Implantable Technology (WIT) lab
 - ENGAGE lab
- Industry summer internships:
 - 2019: Novartis (Switzerland)
@ Digital Solutions
 - 2020: Evidation Health (CA, USA)
@ Digital Measures

Interests – methods for wearable devices data

- Pattern identification and quantification
- Accelerometry data preprocessing
- Physical activity digital measures
- R software development

Interests -- other statistical methods

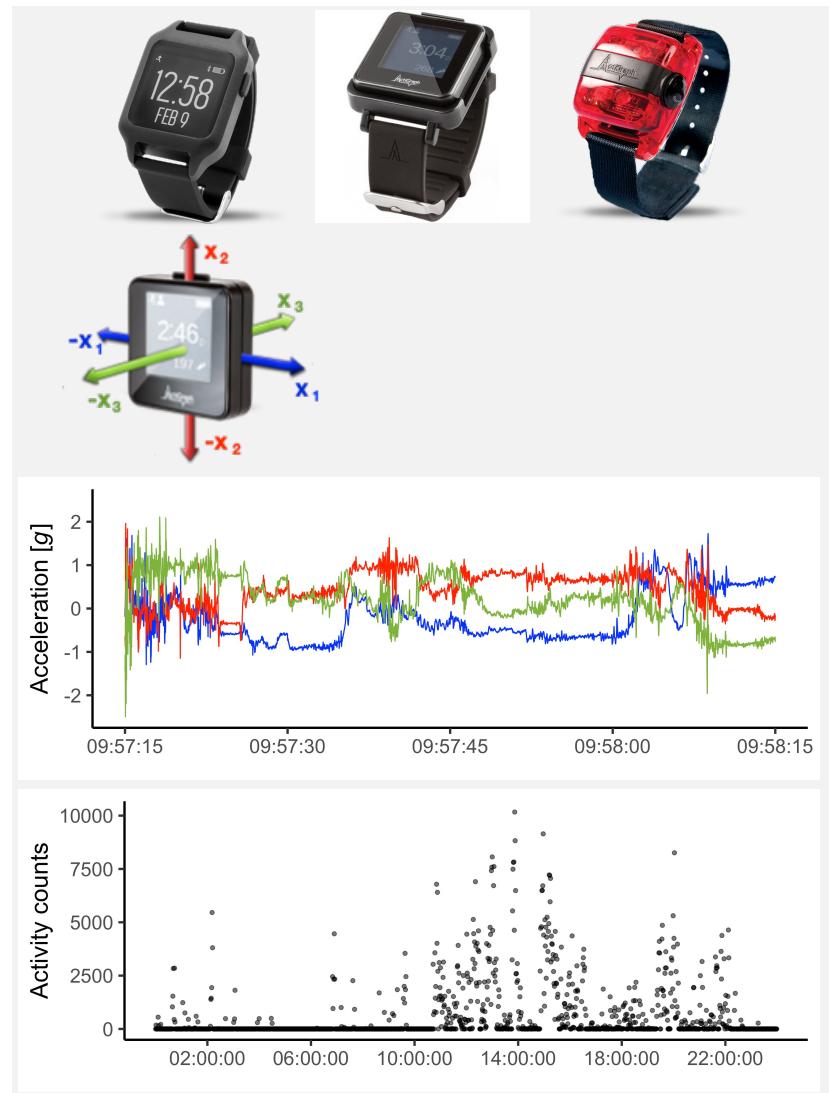
- Power estimation in complex settings
- Regularization, change point detection

Outline

- [16 min] The ADEPT pattern-recognition method with application to walking stride segmentation from raw accelerometry data
- [12 min] Harmonization of accelerometry-based measures of physical activity
- [12 min] The upstrap for power and sample size estimation in complex models

Accelerometry data in health research

- **Wearable monitors** allow for non-invasive, objective monitoring of human motor activity
- **Accelerometer** measures acceleration [g] along three orthogonal axes
- Accelerometry data
 - **Raw data:** three-dimensional time series of acceleration
 - **Summary measures:** raw data aggregated in fixed-time windows (e.g., 1 minute intervals)



Figures rows 1 and 2: ActiGraph, LLC (adapted). Sourced from: <https://actigraphcorp.com/>.

Adaptive empirical pattern transformation (ADEPT) with application to walking stride segmentation

Karas, M., Straczkiewicz, M., Fadel, W., Harezlak, J., Crainiceanu, C. M., Urbanek, J. K. (2019). *Biostatistics*, 22(2), 331–347. <https://doi.org/10.1093/biostatistics/kxz033>

Estimation of free-living walking cadence from wrist-worn sensor accelerometry data and its association with SF-36 quality of life scores

Karas, M., Urbanek, J. K. U., Illiano, V. P., Bogaarts, G., Crainiceanu, C. M., Dorn, J. F. (2021). *Physiological measurement*, 42(6). <https://doi.org/10.1088/1361-6579/ac067b>

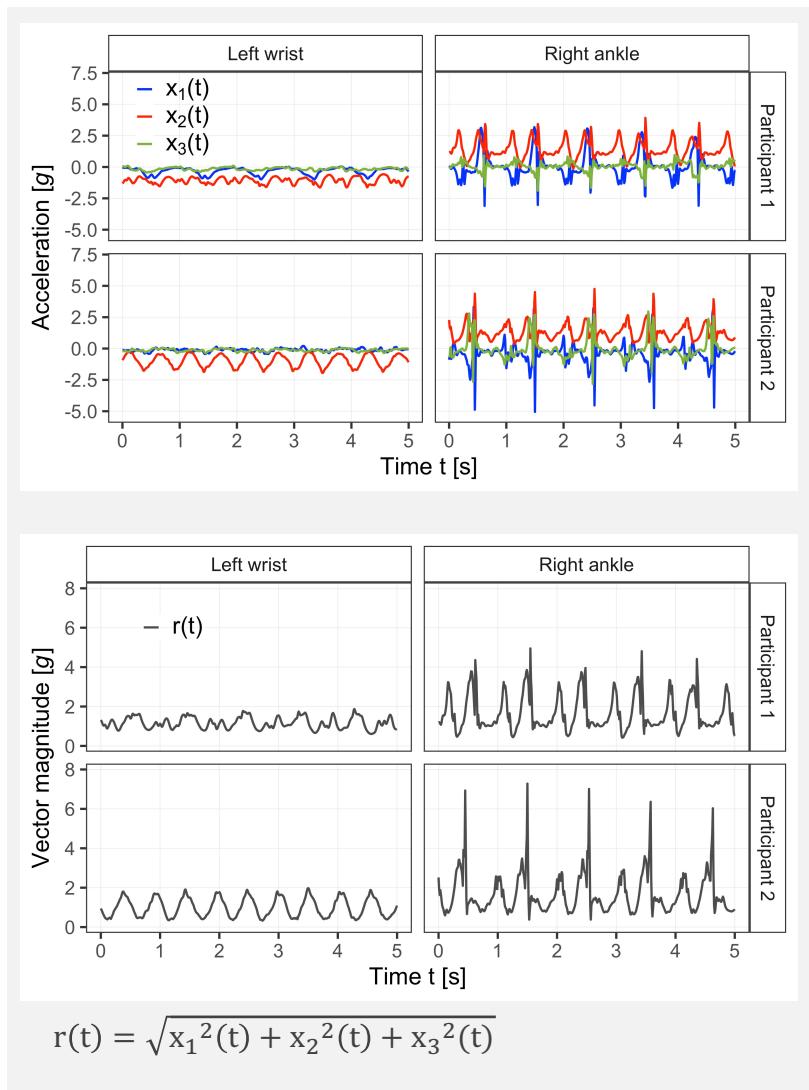
ADEPT: method for automatic, fast and accurate pattern segmentation in time-series

Scientific problem

- Detailed walking characteristics have become increasingly important in health studies
 - Distance covered and speed in a 6 min walk, cadence, stride pattern variability, gait symmetry¹
- Context: supervised and semi-supervised walking
- Need for automatic, fast and accurate methods for walking strides segmentation from raw accelerometry data

Challenges

- Variations in shape and duration of a pattern within and between individuals
- Different sensor locations: wrist (left, right), lower back, hip, ankle



1: Studenski et al., 2011; Brown et al., 2014; Urbanek et al., 2017; Del Din et al., 2019

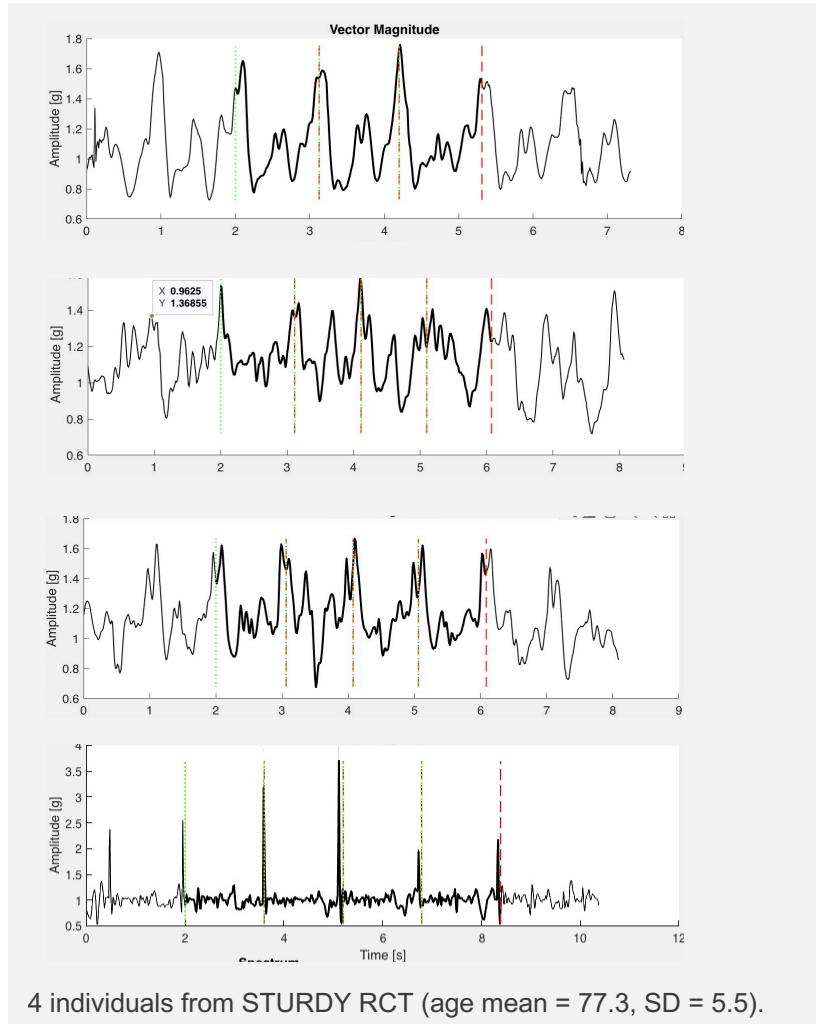
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ADEPT: method for automatic, fast and accurate pattern segmentation in time-series

Proposed method¹: ADaptive Empirical Pattern Transformation (ADEPT)

- Uses a predefined pattern template function $\varphi(t)$ to detect pattern repetitions in the observed data, $x(t)$, by maximizing local similarity (e.g., covariance, correlation) between:
 - a) the collection of time-translated and rescaled templates, $\left\{ \frac{1}{\sqrt{s}} \varphi\left(\frac{t-\tau}{s}\right) \right\}_{s,\tau}$;
 - b) observed data $x(t)$.
- Done by iteratively identifying maxima of similarity (here: covariance) function:

$$W_\varphi(s, \tau) = \int_{-\infty}^{\infty} x(t) \frac{1}{\sqrt{s}} \varphi\left(\frac{t-\tau}{s}\right) dt ,$$

where $\varphi(t)$ is non-zero in $[0,1]$, $x(t)$ is non-zero in $[0, T]$.

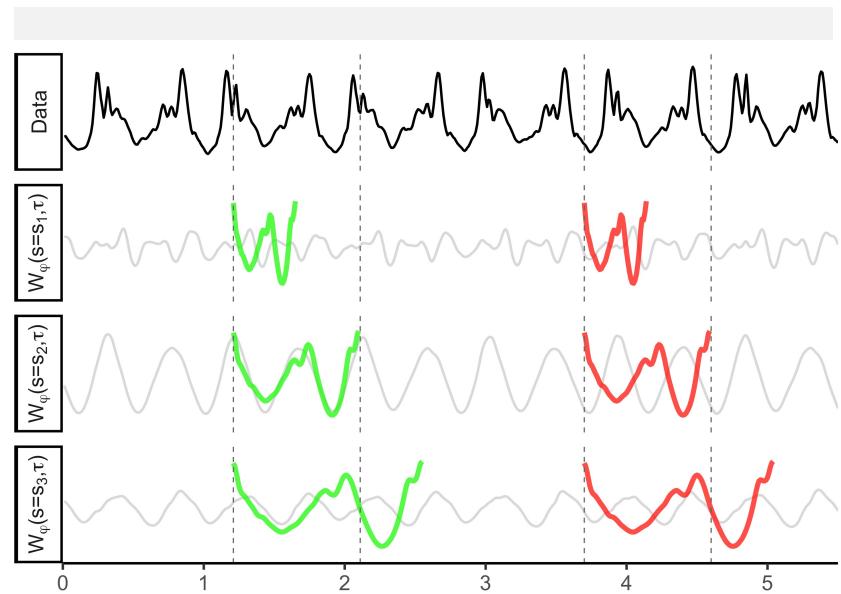
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Optimized for identification of walking strides in raw accelerometry data:

- Uses 1D vector magnitude $r(t)$ of accelerometry data as $x(t)$ => Invariant to sensor rotation, and robust to sensor placement on wrist
- Template $\varphi(t)$ is data-derived, and allows population- or individual-specific templates
- Maximizes $W_\varphi(s, \tau)$ iteratively => Accounts for changes of stride cadence across time
- Allows multiple distinct templates $\varphi_1, \varphi_2, \varphi_3, \dots$ simultaneously => Accounts for changes of stride pattern across time
- Uses location fine-tuning step => Returns precise location of start/end of a stride
- Implementation uses rolling statistics and supports parallel computing => Computational speed

ADEPT: results

ADEPT was **validated** against manual strides segmentation in continuous outdoor walk

- N = 32, healthy adult
- 4 sensor locations (left wrist, left hip, both ankles)
- Excellent agreement with manual segmentation for hip and ankles, very good for wrist

From ADEPT-segmented walking strides:

- Estimated **temporal cadence** [steps/s] trajectory
- Estimated **subject-specific stride patterns**

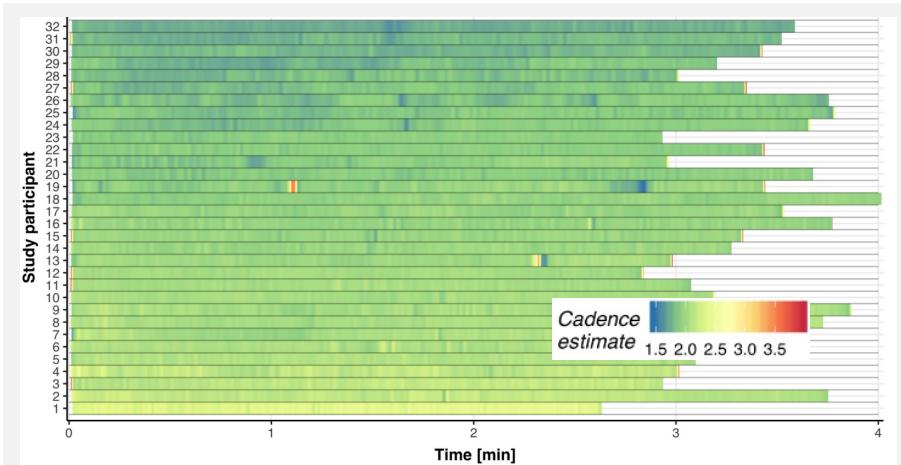


Figure 1. Walking cadence [steps/s] estimates during continuous outdoor walk (N = 32), based on raw accelerometry data collected at left ankle¹.

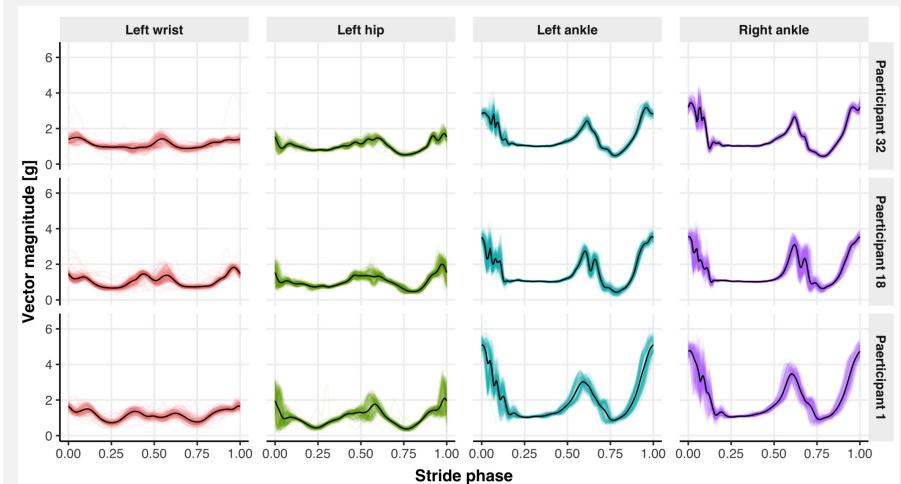


Figure 2. Examples of subject- and sensor-location specific stride patterns for three selected study participants¹.

ADEPT extension: walking segmentation from data collected in the free-living at a wrist

Scientific problem

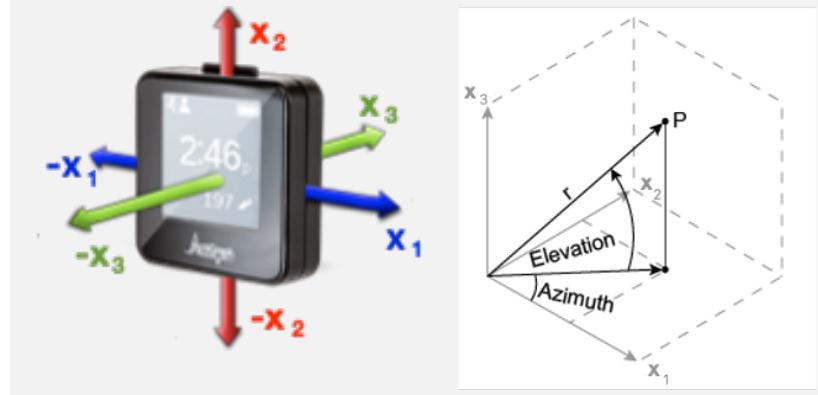
- Walking features measured **in the lab are weakly associated with those from the free-living¹**
- Free-living: decreased speed, increased step variability, increased asymmetry¹
- Need for methods to **segment walking strides in the free-living environment**

Challenges

- Sensor typically worn at wrist -- a challenging location for walking identification
- Validation is difficult

Proposed method²

- Use ADEPT for initial exhaustive segmentation of walking stride patterns
- Filter the results — accept a pattern if:
 - (a) has high correlation with a template,
 - (b) in consecutive ≥ 3 ,
 - (c) “looks alike” its neighbouring patterns
- For (c), uses transformation of raw accelerometry data from Cartesian $[x_1, x_2, x_3]$ into spherical $[az, el, r]$ coordinate system



1: Del Din et al., 2016; Mueller et al., 2019; Van Ancum et al., 2019

2: Karas et al., 2021

Figure -- left: ActiGraph (adapted), LLC. Figure – right: MathWorks (adapted).

ADEPT: summary of contributions

Methods

- **Karas et al. (2019)**. Adaptive empirical pattern transformation (ADEPT) with application to walking stride segmentation. *Biostatistics*.
- **Karas et al. (2021)**. Estimation of free-living walking cadence from wrist-worn sensor accelerometry data and its association with SF-36 quality of life scores. *Physiological Measurement*.

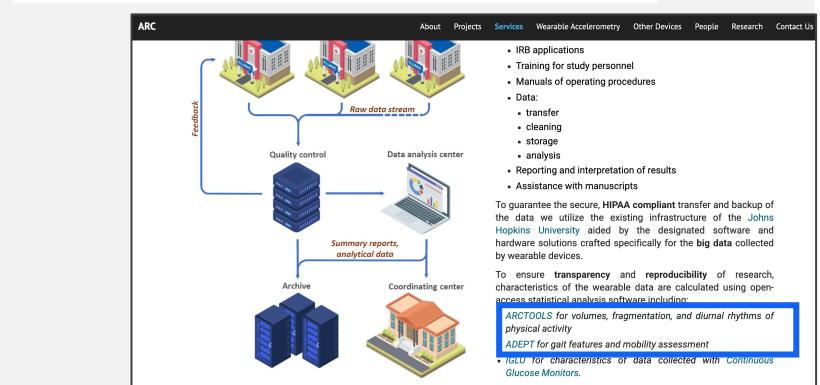
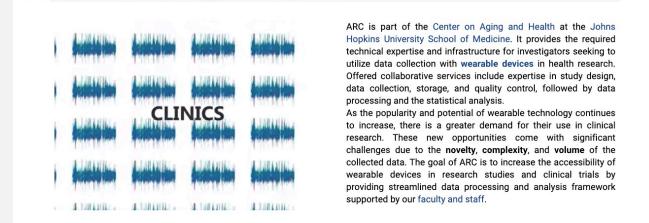
Applications

- **Karas et al. (2021)**: higher free-living cadence associated with better quality of life score
- **Urbanek et al.** (revised, resubmitted): higher free-living cadence associated with lower fall rates in older individuals
- **Catallini (2020)**: In MS thesis, ADEPT used for segmentation of neuronal activity traces from time series of calcium imaging
- **Rubin lab (U of Chicago)**: Integrating ADEPT for iOS for semi-supervised experiments
- **Qiao (U of Pittsburgh; PhD thesis)**: novel markers to identify performance fatigability during a fast-paced 400 m walk

Resources

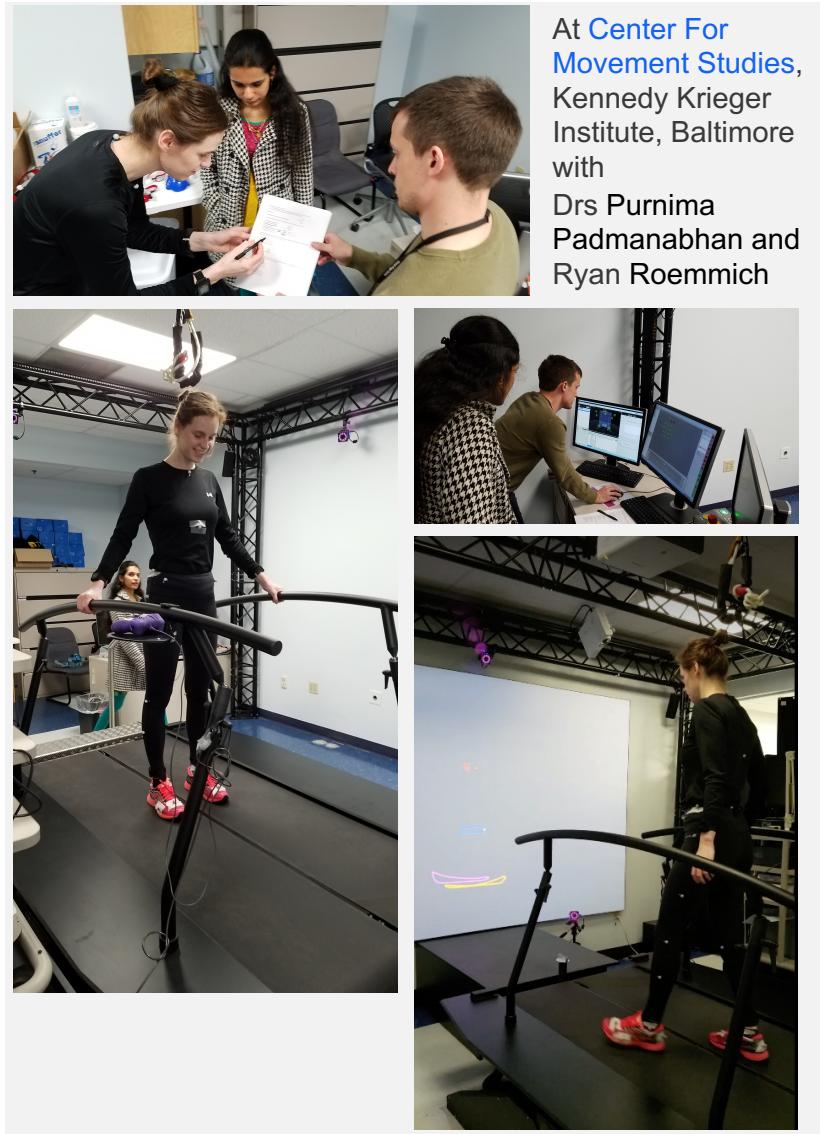
- adept R package:
 - Implements ADEPT and its extension for free-living
 - Data examples and tutorials

<https://www.accelerometry.org/>



ADEPT: potential future directions

1. Functional registration of individual walking stride patterns (characterization of gait asymmetry etc.)
2. Functional registration of temporal walking characteristics from standardized tests (e.g. cadence in 6 minute walk test)



Harmonization of accelerometry-based measures of physical activity

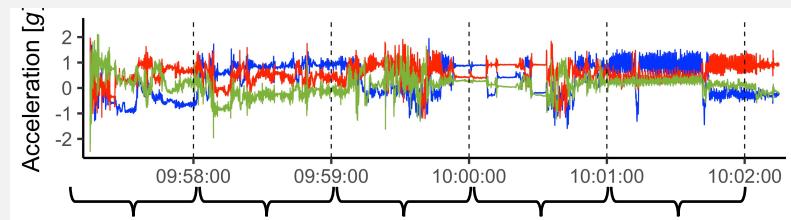
Karas, M.*, Muschelli, J. *, Leroux, A., Urbanek, J.K., Wanigatunga, A.A., Bai, J., Crainiceanu, C.M., Schrack, J.A. (2021). Submitted.

* : Shared co-first authorship.

Harmonization of open-source and proprietary accelerometry-based physical activity measures

Scientific problem

- Summary measures of raw accelerometry data are commonly used in health research¹ to characterize physical activity
- Widely-used: ActiGraph “activity counts” (**AC**)
 - ActiGraph hardware and licensed software needed to derive from raw data
- Recently, open-source statistics have been proposed to aggregate raw data: **MIMS**, **ENMO**, **MAD**, **AI**²
- Comparability to previously published research is unknown
 - AC** cut-off points, **AC** population quantiles



Measure	Based on
MIMS	AUC of interpolated, extrapolated, bandpass-filtered $x_m(t)$; then added across axes $m = 1,2,3$
ENMO	Mean of $r(t)$ vector magnitude from pre-calibrated raw data $[x_1(t), x_2(t), x_3(t)]$
MAD	Mean amplitude deviation of $r(t)$ vector magnitude
AI	Variance of $x_m(t)$; then averaged across axes $m = 1,2,3$

MIMS -- Monitor-Independent Movement Summary

ENMO -- Euclidean Norm Minus One

MAD -- Mean Amplitude Deviation

AI -- Activity Index

1: Karas et al., 2019b.

2: MIMS: John et al., 2019; ENMO: van Hees et al., 2013; MAD: Vähä-Ypyä et al., 2015; AI: Bai et al., 2012

Harmonization of open-source and proprietary accelerometry-based physical activity measures

Contributions

Data from ~700 participants in the Baltimore Longitudinal Study on Aging (BLSA), each monitored for a week with a wrist-worn PA sensor

1. Summarized raw data at minute-level: **AC** and open-source **MIMS**, **ENMO**, **MAD**, **AI**
2. Quantified association between **AC** and open-source measures marginally and conditionally on age, sex and BMI
3. Harmonized minute-level **AC** with open-source measures via one-to-one mapping
4. Reproduced some of the published BLSA results that used **AC** with the use of the open-source measures

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Challenges

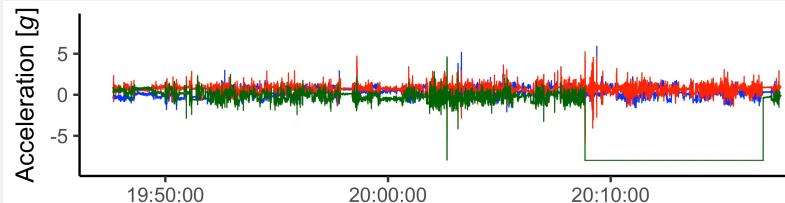
- Large volume of raw accelerometry data needs quality check
 - 700 participants x 7 days x 1440 minutes x 60 seconds x 80 obs./s x 3 sensor axes = **101,606,400,000** (one hundred billion+)

Methods

- Adapted raw data quality flags from recently published NHANES protocol¹
- Implemented flags to detect acceleration spikes, values at the sensor's dynamic range

Results

- Identified few flagged cases of raw measurements



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Methods

- Linear regression with subject-specific correlation between measures as an outcome

Results

- Very high correlation between: AC and MIMS, AC and AI
- Significant but small effects of covariate(s)

	Unadjust. model	Model adjusted for: age, BMI, sex				
		Intercept	Intercept	Age	BMI	Sex (is male)
Response var.	Coef. est. (se)	Coef. est. (se)	Coef. est. (se)	Coef. est. (se)	Coef. est. (se)	Coef. est. (se)
corr (AC, MIMS)	0.988 (0.0002)	0.988 (0.0017)	< 0.001 (<0.0001)	< 0.001 (<0.0001)	-0.002 (0.0005)*	
corr (AC, ENMO)	0.867 (0.0018)	0.887 (0.0138)	-0.001 (0.0001)*	0.001 (0.0004)	> -0.001 (0.0037)	
corr (AC, MAD)	0.913 (0.0013)	0.892 (0.0099)	< 0.001 (0.0001)	0.001 (0.0003)*	-0.010 (0.0026)*	
corr (AC, AI)	0.970 (0.0007)	0.962 (0.0050)	< 0.001 (< 0.0001)	< 0.001 (0.0001)*	-0.010 (0.0013)*	

Table. ** symbol is used to denote model coefficients (excluding intercept) for which the corresponding p-value was <0.05.

Harmonization of open-source and proprietary accelerometry-based physical activity measures

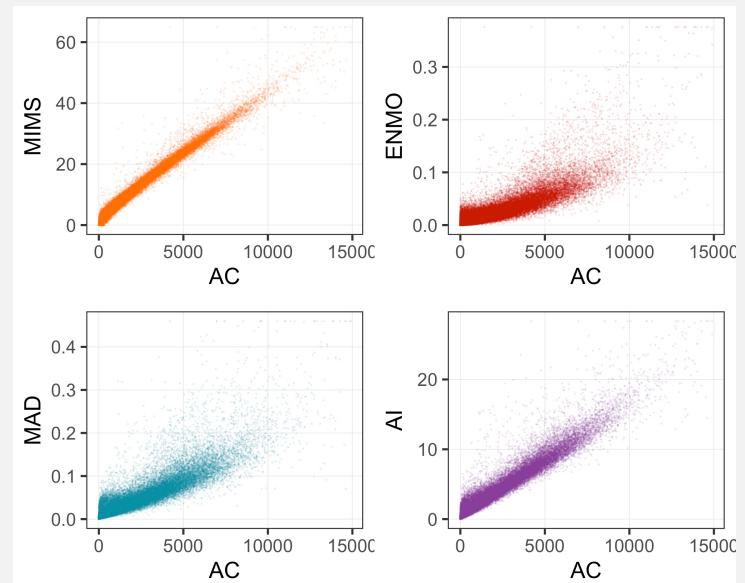
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Challenges

- Estimate the relation between pairs of minute-level measures ($x_{ij}(t), y_{ij}(t)$) e.g., ($AC_{ij}(t), MIMS_{ij}(t)$) as a smooth function f while accounting for correlation structure (i-th participant, j-th day, t-th minute)
- Volume of minute-level data = 700 participants x 7 days x 1440 minutes = **7,056,000**



Showing 1% of the data.

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Methods

- Estimated f via additive model $y_{ij}(t) = f(x_{ij}(t)) + \varepsilon_{ij}(t)$, assuming independence
- Used "case bootstrap"¹ (sampling units at the highest level and then sampling within these units without replacement) to get 95% CI for \hat{f}
- Used \hat{f} to define one-to-one harmonization mapping
- Evaluated \hat{f} in tasks of: (a) predicting total AC, (b) classifying a minute into active vs non-active

1: Ren et al., 2010

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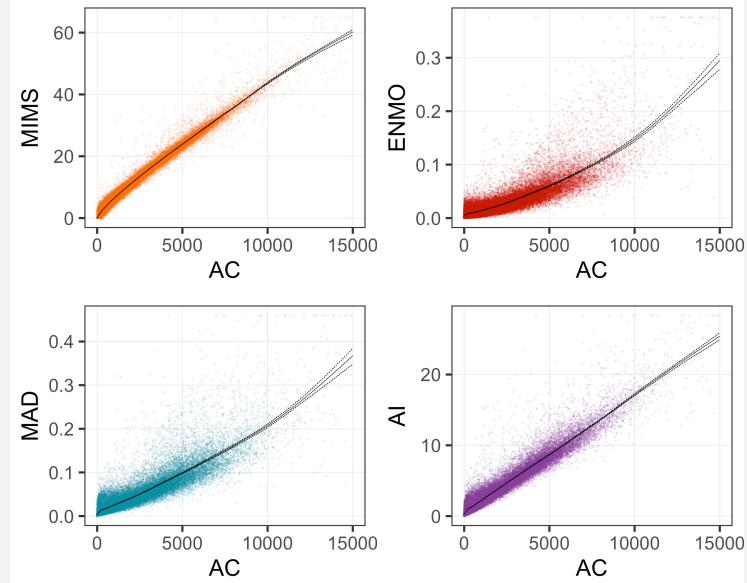
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Results

Black solid line: $\hat{f}(AC)$, dashed lines: 95% CI



AC cut-off proposed in	AC	$\hat{f}_{MIMS}(AC)$ (95% CI)
Koster (2016)	1853	10.56 [10.53, 10.59]
Montoye (2020)	2860	15.05 [15.02, 15.07]
Montoye (2020)	3940	19.61 [19.58, 19.65]

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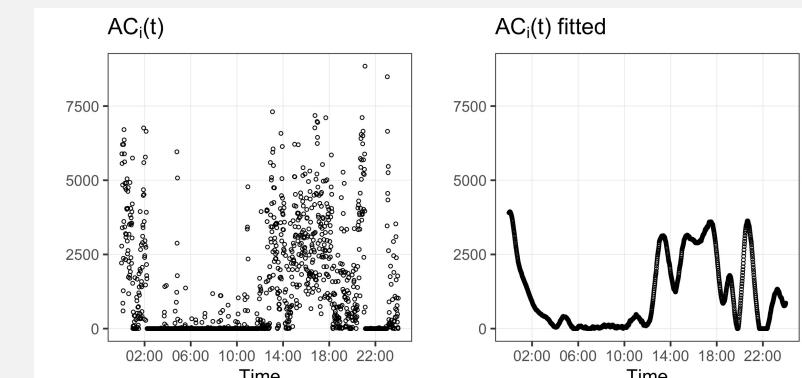
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Challenges

- Required to impute minute-level data missingness (up to 10% per 24 h)

Methods

- For each measure separately, use FPCA model $\mathbf{Y}_i(t) = \mu(t) + \sum_{k=1}^{ncp} \xi_{ik} \phi_k(t) + \varepsilon_i(t)$ to estimate $\hat{\mathbf{Y}}_i(t)$ -- smoothed (fitted) version of each i -th participant-day functional observation¹
- Use $\hat{\mathbf{Y}}_i(t)$ for imputation



1: Leroux et al., 2020

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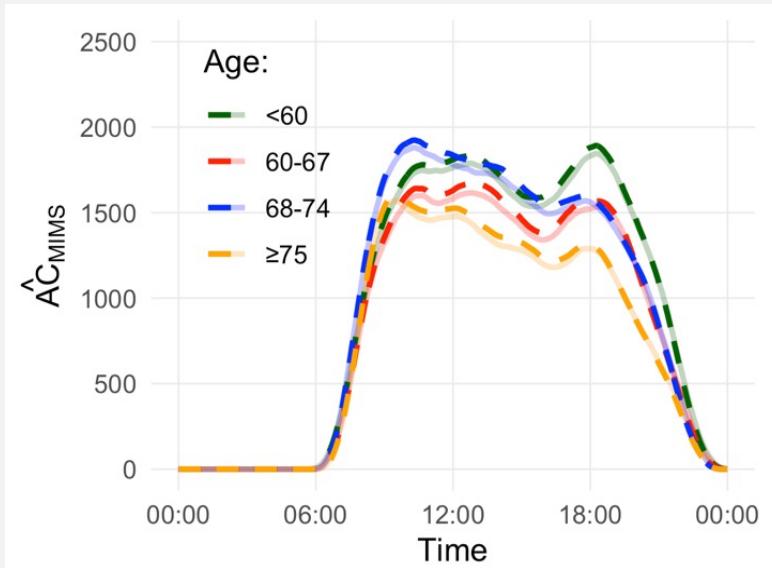


Figure. Smoothed 24-hour median activity counts per minute across four age group. Solid semi-transparent colour lines: AC. Dashed colour lines: results obtained with \widehat{AC} values mapped into AC from MIMS using the harmonization mapping.

1: Schrack et al., 2013

Summary measures of physical activity: potential future directions

1. Harmonization of data from large- and mega-size studies collecting minute-level measurements of physical activity
2. Data imputation for continuously collected measurements of physical activity



BLSA BALTIMORE LONGITUDINAL STUDY OF AGING

AC



nhats

National Health & Aging Trends Study

how daily life changes as we age

AC



biobank uk

Improving the health of future generations

ENMO



NHANES

National Health and Nutrition Examination Survey

MIMS

NHANES most recent release (cohorts 2011-2012, 2013-2014)

Upstrap for estimating power and sample size in complex models

Karas, M., Crainiceanu, C.M. (2021). Submitted.
<https://doi.org/10.1101/2021.08.21.457220>

Upstrap method for power and sample size estimation in complex models

Scientific problem

Given an observed data **sample x** of sample **size N** , a null and an alternative hypothesis and a test statistic, assuming significance level α ,

- estimate the sample size M required to achieve power $(1 - \beta)$ (i.e., to achieve probability of rejecting the null hypothesis when the null is true)

Here, we consider power to detect:

- (a) an effect size observed in the sample x ;
- (b) an effect size chosen by a researcher.

and aim to address complex settings, including testing significance of model coefficients in:

LM, GLM, LMM, GLMM.

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```
# Example: one-sample t-test

set.seed(123)

# simulate observed sample
x <- rnorm(n = 30, mean = 0.2, sd = 1)

mean(x)
# [1] 0.1528962

# effect size observed in sample x
# ("observed power" estimation)
power.t.test(n = 30, delta = mean(x),
  sd = sd(x), type = "one.sample")$power
# [1] 0.1283329
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# effect size chosen by researcher
# (here: 0.1)
power.t.test(n = 30, delta = 0.1,
  sd = sd(x), type = "one.sample")$power
# [1] 0.07781938
```

Upstrap method for power and sample size estimation in complex models

Methods

- Upstrap -- **resampling with replacement fewer or more observations** than in original sample **x** -- was proposed¹ as a general solution
 - For effect size observed in the sample **x**
 - Not evaluated in numerical experiments
- Contributions of this project:
 - Extend upstrap approach for estimating power to detect an effect size chosen by a researcher
 - Evaluate method in a simulation study

```
# Example: bootstrap vs upstrap

# observed sample
x <- 1:10

# bootstrap resample
xb <- sample(x, size = 10, replace = TRUE)

# upstrap resample
# (sample size larger than in original x)
xu1 <- sample(x, size = 20, replace = TRUE)

# upstrap resample
# (sample size smaller than in original x)
xu2 <- sample(x, size = 8, replace = TRUE)
```

Upstrap-based algorithm for estimating power

Methods

Given observed data sample x of size N , to estimate power for a target sample size M :

- Case (a): effect size observed in the sample x
 1. Generate B upstrap resamples of size M ;
 2. Perform hypothesis test on each resample;
 3. Estimate power as the proportion of B resamples where the null hypothesis was rejected.
- Case (b): effect size chosen by researcher
 - As above (a), but update response variable values in sample x (/resample) so as the updated sample (/resample) reflects the target effect size¹

1: Details in the preprint

Upstrap-based algorithm for estimating power

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Toy example: one-sample t-test

```
# simulate observed sample
x <- rnorm(n = 30, mean = 0.2, sd = 1)

# Case (a): effect size observed

out <- rep(NA, B)
for (bb in 1 : B){
  x_bb <- sample(x, size = M, replace = T)
  out[bb] <- (t.test(x_bb)$p.value < 0.05)
}
mean(out)
```

Upstrap-based algorithm for estimating power

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# Case (a): effect size observed

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for (bb in 1 : B){
  x_bb <- sample(x, size = M, replace = T)
  out[bb] <- (t.test(x_bb)$p.value < 0.05)
}
mean(out)

# Case (b): effect size chosen to 0.4

x <- x + (0.4 - mean(x))
out <- rep(NA, B)
for (bb in 1 : B){
  x_bb <- sample(x, size = M, replace = T)
  out[bb] <- (t.test(x_bb)$p.value < 0.05)
}
mean(out)
```

Upstrap-based algorithm for estimating power

Methods

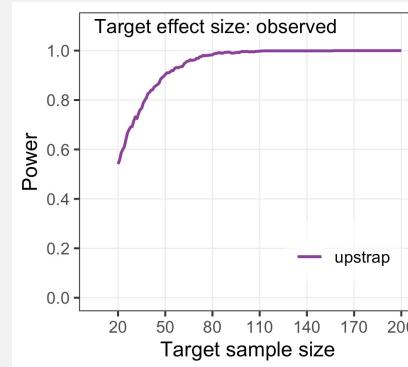
Given observed data sample x of size N , to estimate power for a target sample size M :

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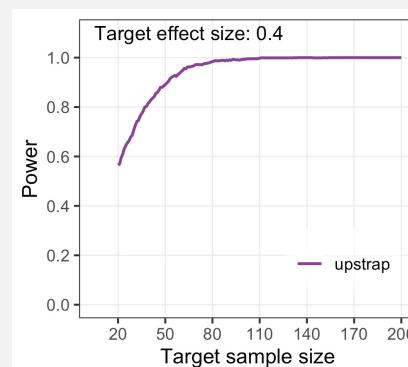
Toy example: one-sample t-test

Consider: $x_i \sim_{\text{iid}} \mathcal{N}(0.3, 1)$, $i = 1, \dots, 50$, 1 repetition

Case (a)



Case (b)



Upstrap-based algorithm for estimating power

Methods

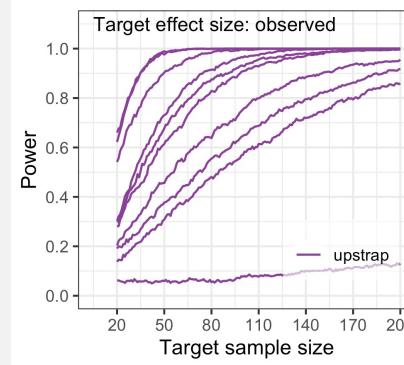
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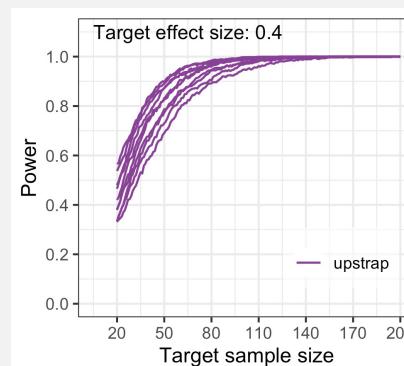
Toy example: one-sample t-test

Consider: $x_i \sim_{\text{iid}} \mathcal{N}(0.3, 1)$, $i = 1, \dots, 50$, **15 repetitions**

Case (a)



Case (b)



Upstrap-based algorithm for estimating power

Methods

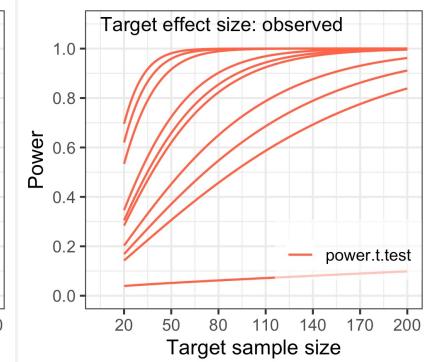
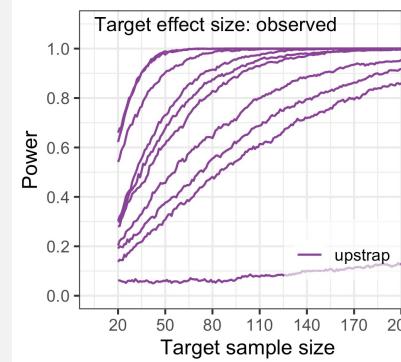
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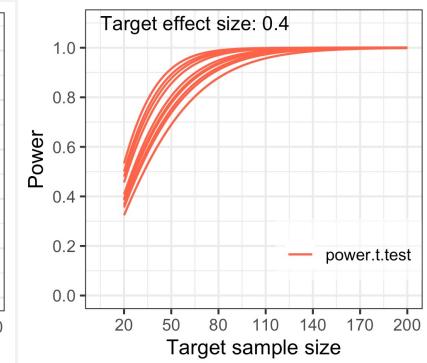
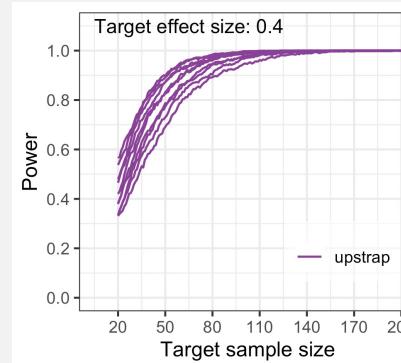
Toy example: one-sample t-test

Consider: $x_i \sim_{\text{iid}} \mathcal{N}(0.3, 1)$, $i = 1, \dots, 50$, 15 repetitions

Case (a)



Case (b)



Upstrap-based algorithm for estimating power

Methods

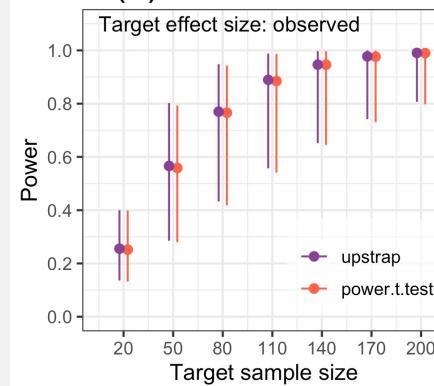
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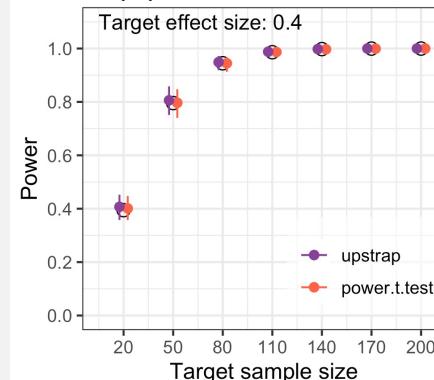
Toy example: one-sample t-test

Consider: $x_i \sim_{\text{iid}} \mathcal{N}(0.3, 1)$, $i = 1, \dots, 50$, 1000 repetitions, aggregated power values (mean, 25th and 75th percentiles)

Case (a)



Case (b)



Upstrap-based algorithm for estimating power: simulation study

- Summary of the simulation setup across six different problems:

	Data-generating model (effect being tested highlighted in color)	Observed sample size	Target effect size	Comparator to upstrap
1	$Y_i = \beta_0 + \varepsilon_i$	50	0.3, 0.4, observed	power.t.test()
2	$Y_i = \beta_0 + \beta_1 X_{1i} + \varepsilon_i$	50	0.3, 0.4, observed	power.t.test()
3	$Y_i = \beta_0 + \beta_1 X_{1i} + \beta_2 X_{2i} + \beta_3 X_{3i} + \varepsilon_i$	50	0.5, 1, observed	SIMR
4	$\text{logit}(\pi_i) = \beta_0 + \beta_1 X_{1i} + \beta_2 X_{2i} + \beta_3 X_{3i}$	50	0.5, 1, observed	SIMR
5	$Y_{ij} = b_{0i} + \beta_0 + \beta_1 X_{1ij} + \beta_2 X_{2ij} + \beta_3 X_{3ij} + \varepsilon_{ij}$	50	0.5, 1, observed	SIMR
6	$\text{logit}(\pi_{ij}) = b_{0i} + \beta_0 + \beta_1 X_{1ij} + \beta_2 X_{2ij} + \beta_3 X_{3ij}$	50	0.5, 1, observed	SIMR

- In each of the six problems:
 - X_{1i} / X_{1ij} is defined as **dichotomous** variable
 - 1,000 independent experiment repetitions (generating a sample and power estimation)
 - Two-sided test used to test $H_0: \beta = 0$ versus $H_1: \beta \neq 0$ at significance level $\alpha = 0.05$
 - “True power”** estimated by proportion of null rejected from 10,000 samples

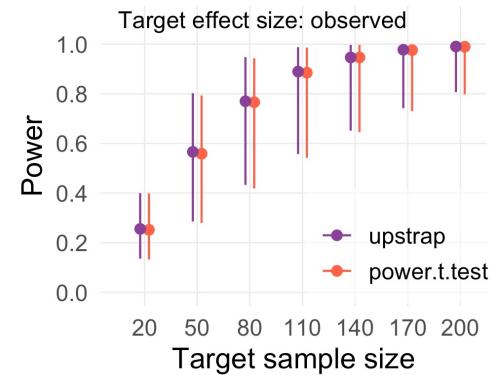
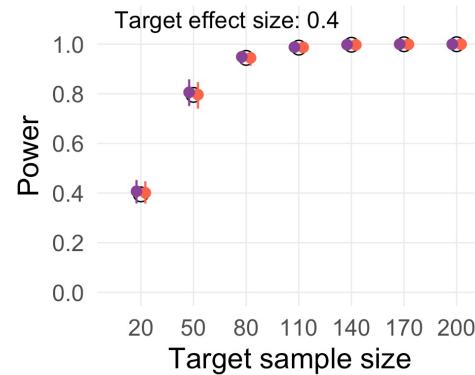
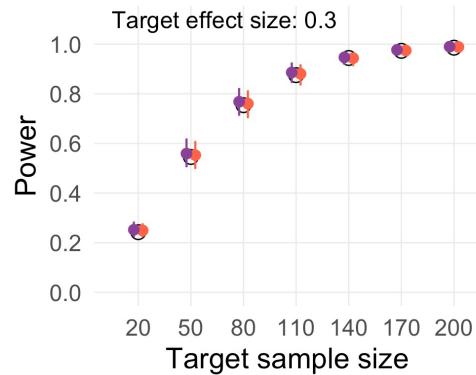
Upstrap-based algorithm for estimating power: simulation study

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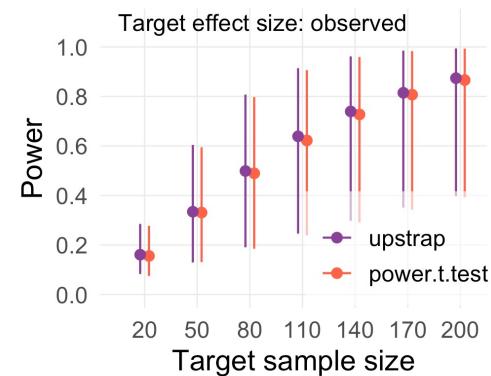
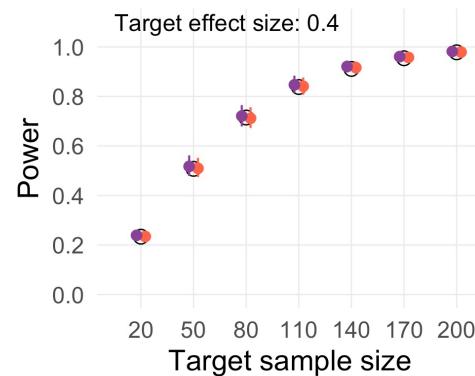
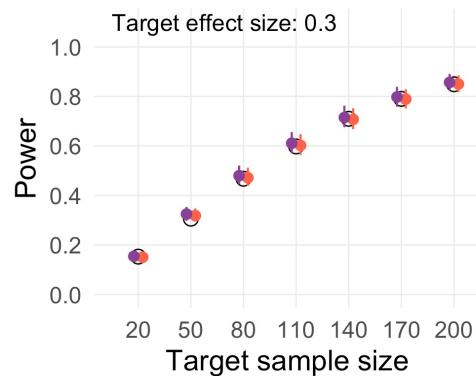
	Data-generating model (effect being tested highlighted in color)	Observed sample size	Target effect size	Comparator to upstrap
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3	$Y_i = \beta_0 + \beta_1 X_{1i} + \beta_2 X_{2i} + \beta_3 X_{3i} + \varepsilon_i$	50	0.5, 1, observed	SIMR ¹
4	$\text{logit}(\pi_i) = \beta_0 + \beta_1 X_{1i} + \beta_2 X_{2i} + \beta_3 X_{3i}$	50	0.5, 1, observed	SIMR
5	$Y_{ij} = b_{0i} + \beta_0 + \beta_1 X_{1ij} + \beta_2 X_{2ij} + \beta_3 X_{3ij} + \varepsilon_{ij}$	50	0.5, 1, observed	SIMR
6	$\text{logit}(\pi_{ij}) = b_{0i} + \beta_0 + \beta_1 X_{1ij} + \beta_2 X_{2ij} + \beta_3 X_{3ij}$	50	0.5, 1, observed	SIMR

- In each of the six problems:
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 - “True power” estimated by proportion of null rejected from 10,000 samples

Simulation problem 1



Simulation problem 2



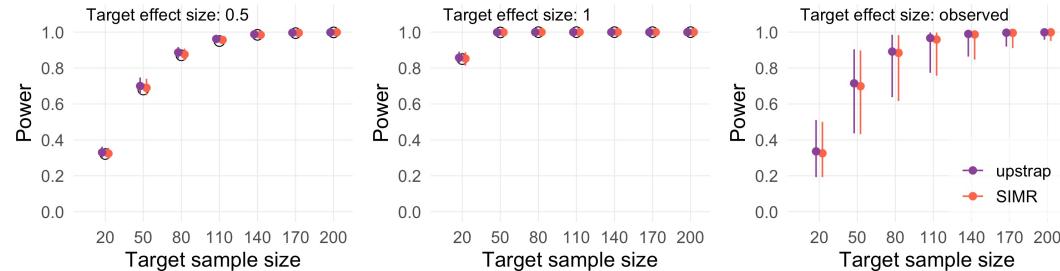
Upstrap-based algorithm for estimating power: simulation study

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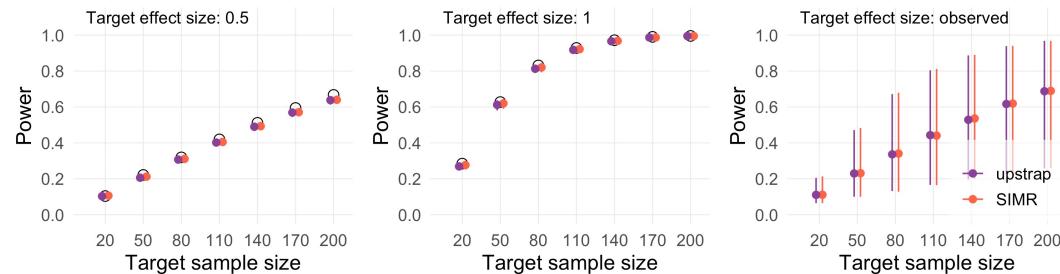
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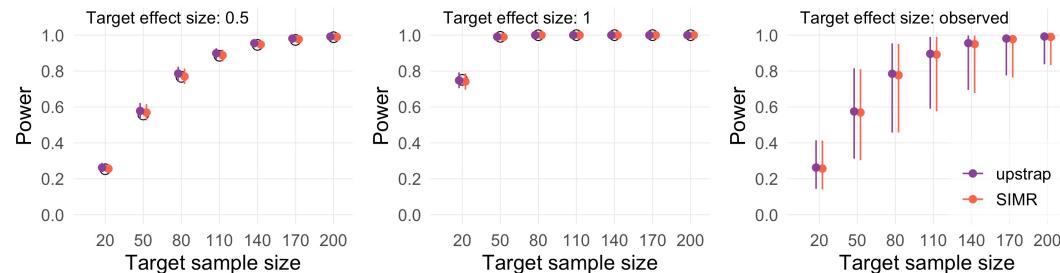
Simulation problem 3



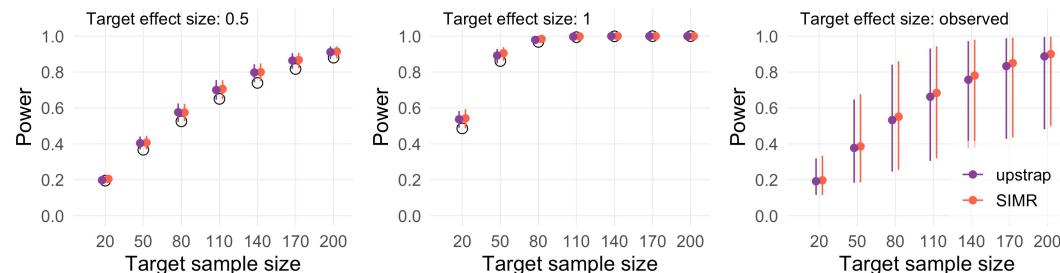
Simulation problem 4



Simulation problem 5



Simulation problem 6



Upstrap-based algorithm for estimating power: summary

- Simulation results:
 - For one- and two-sample t-test, the upstrap performed essentially identical to the well-established analytical solutions for power estimation
 - In complex scenarios, the upstrap performed similarly to the existing method from SIMR R package; both approaches demonstrated very high agreement with the true power estimates
- The upstrap method is “read-and-use”
 - It can be implemented by any analyst who is familiar with software allowing to: (a) resample data, (b) run the statistical test of interest

Upstrap method for power and sample size estimation: potential future directions

1. Upstrap for estimating power to detect an effect while
 - (a) preserving or (b) changing covariate class proportions
2. Resampling (up/down) cluster-specific observations in longitudinal data

Summary of contributions

The main methodological contributions of this thesis are:

1. development and validation of ADEPT, a novel statistical pattern-segmentation method;
2. introduction of harmonization methods of objective summary measures of physical activity;
3. study of the upstrap properties in complex scenarios;
4. development of four R software packages.

R software packages:

- **runstats**: Fast Computation of Running Statistics for Time Series ([CRAN](#))
- **adept**: Adaptive Empirical Pattern Transformation ([CRAN](#))
- **adeptdata**: Accelerometry Data Sets ([CRAN](#))
- **arctools**: Processing and Physical Activity Summaries of Minute Level Activity Data ([CRAN](#))

All projects code publicly available:

- ADEPT ([GitHub repo 1](#), [GitHub repo 2](#))
- Harmonization of measures ([GitHub repo](#))
- Upstrap ([GitHub repo](#))

Reviewer for:

- Plos One, Digital Biomarkers, Scandinavian Journal of Medicine & Science in Sports ([Publons](#))

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* : Shared co-first authorship.

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