

# B<sub>1</sub>-Sensitivity Analysis of qMT

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## Introduction

- B<sub>1</sub> mapping is an important measurement used to correct the excitation flip angle and MT saturation powers in pulsed quantitative magnetization transfer (qMT) imaging.
- Additional measurements necessary for qMT (e.g. T<sub>1</sub> mapping) may also require B<sub>1</sub> maps. For example, variable flip angle (VFA) T<sub>1</sub> mapping requires B<sub>1</sub> maps, while inversion recovery (IR) typically does not<sup>1</sup>.
- Local (e.g. artifacts) or global (e.g. systemic biases) inaccuracies in B<sub>1</sub> mapping<sup>2</sup> will propagate to the fitted qMT parameters differently, depending on the T<sub>1</sub> method.**
- We present a simulation-based analysis of the B<sub>1</sub> sensitivity of pulsed qMT, investigating the propagation of the B<sub>1</sub> error to the qMT parameters using different T<sub>1</sub> mapping methods (VFA vs. IR).
- We demonstrate the pool-size ratio F is robust against B<sub>1</sub> inaccuracies when VFA T<sub>1</sub> mapping is used, but this comes at the cost of an increase in error in the exchange rate kf.

## Methods

- Pulsed MT SPGR signals were simulated in MATLAB (MATLAB2011a, The Mathworks Inc.) using the Sled and Pike approximations<sup>4</sup>.

### Healthy WM qMT Tissue Parameters

- F = 0.122
- kf = 3.97 s<sup>-1</sup>
- R<sub>1f</sub>, R<sub>1r</sub> = 1.11, 1.0 s<sup>-1</sup>
- T<sub>2f</sub>, T<sub>2r</sub> = 27.2 ms, 10.96 μs

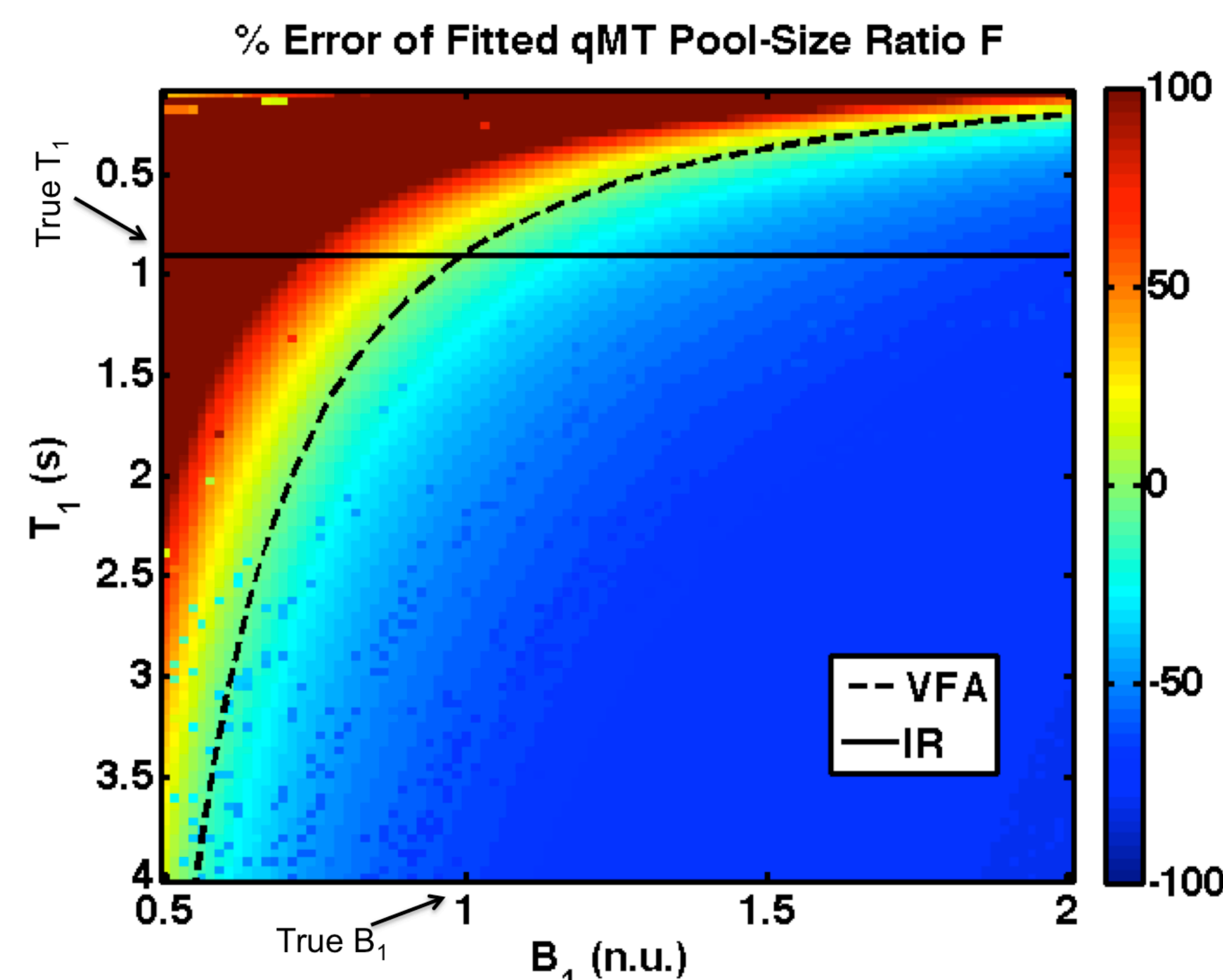
### qMT Protocol (SPGR)

- TR = 25 ms
- α<sub>excitation</sub> = 7°
- Gaussian-Hanning MT pulses
  - Pulse duration = 10.2 ms
  - α<sub>MT</sub> = 142° and 426°
  - Off-resonance frequencies (for each α<sub>MT</sub>) = 423.9 Hz, 1,087.5 Hz, 2,731.6 Hz, 6,861.6 Hz, and 17,235.4 Hz.

### Data Fitting

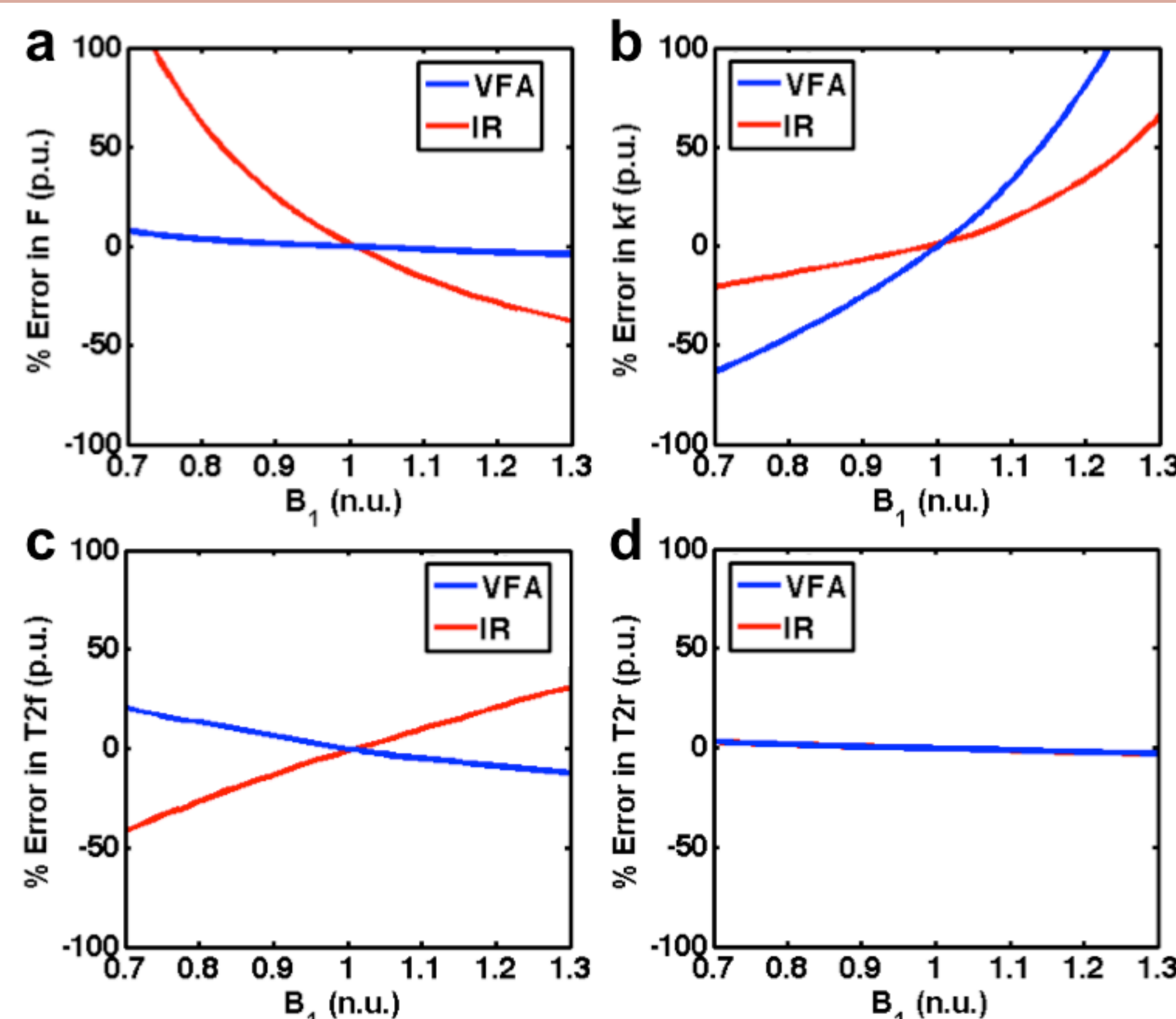
- The qMT signal was subsequently fitted<sup>5</sup> for 10,000 B<sub>1</sub> and T<sub>1</sub> value combinations.
  - T<sub>1</sub> varied independently of B<sub>1</sub> for this step (without any assumptions on the measurement method.).
  - 100 B<sub>1</sub> values between 0.5 to 2 (B<sub>1,true</sub> = 1).
  - 100 T<sub>1</sub> value between 0.1 s to 4 s (T<sub>1,true</sub> = 0.9 s).
- qMT was also fitted using T<sub>1</sub> from simulated VFA signals<sup>1</sup>:
  - TR = 25 ms, α = 3° and 20°, T<sub>1</sub> = T<sub>1,true</sub>
  - T<sub>1</sub> values were fitted from the VFA data using each B<sub>1</sub> error value.

## Results – B<sub>1</sub> vs. T<sub>1</sub>



**Figure 1.** Percent error in fitted qMT F values in the presence of a wide range of B<sub>1</sub> and T<sub>1</sub> errors (B<sub>1,true</sub> = 1 n.u., T<sub>1,true</sub> = 0.9 s).

## Results – VFA vs. IR



**Figure 2.** Percent error in fitted qMT parameters for a range of B<sub>1</sub> errors (a – pool size ratio (F), b – magnetization exchange rate (kf), c – free pool T2 (T<sub>2f</sub>), d – restricted pool T2 (T<sub>2r</sub>)). See solid and dashed lines in Fig. 1 for the B<sub>1</sub>-dependence of VFA (solid) and IR (dashed) T<sub>1</sub>.

## Results

- The superimposed lines in Fig. 1 show the range of errors in the fitted pool-size ratio F using a B<sub>1</sub>-independent T<sub>1</sub> method (e.g. IR) (solid line), and from VFA T<sub>1</sub> mapping (dashed line).
- Figure 2 shows the errors in fitted qMT parameters (F, kf, T<sub>2f</sub>, T<sub>2r</sub>) using B<sub>1</sub>-independent (IR) and VFA-measured T<sub>1</sub> for a range of B<sub>1</sub> inaccuracies that may be observed in vivo.
- Errors in F induced by B<sub>1</sub> errors were greatly reduced by using VFA T<sub>1</sub> mapping (Fig. 2a - blue).
- A substantial increase in errors of kf occurs for VFA relative to IR (Fig. 2b - blue), while T<sub>2r</sub> remains insensitive to B<sub>1</sub> inaccuracies for both cases.

## Discussion

- The qMT pool-size ratio F was shown to be nearly B<sub>1</sub>-error insensitive when using VFA T<sub>1</sub> mapping (Fig. 2a - blue).
- Using a B<sub>1</sub>-independent T<sub>1</sub> measure, such as IR, produces large qMT F errors (>100% to -45% for B<sub>1</sub> errors between ±30%, Fig. 2a - red). VFA T<sub>1</sub> mapping kept qMT F errors within a moderate range (7% to -3%, Fig. 2a - blue).
- These results suggest that, when investigating the pool-size ratio (a biomarker for white matter myelin density), VFA T<sub>1</sub> mapping should be used in the pulsed qMT protocol to reduce the effects of B<sub>1</sub> inaccuracies.
- For applications of qMT where kf is the biomarker of interest (e.g. cartilage imaging<sup>6</sup>, systemic inflammation<sup>7</sup>), our results suggest that a B<sub>1</sub>-independent measure of T<sub>1</sub> may be preferable instead of the VFA method (Fig. 2b - red).

## Summary

- This work demonstrated that pulsed qMT pool-size ratio F maps fitted using VFA T<sub>1</sub> are nearly insensitive to B<sub>1</sub> inaccuracies.
- Under certain circumstances, B<sub>1</sub> mapping could be omitted altogether without substantial bias to F values.
- Pulsed qMT using B<sub>1</sub>-independent measures of T<sub>1</sub> (e.g. IR) may be better suited for MT exchange rate (kf) mapping.
- Further sensitivity analysis of the qMT equations for different measurement protocols could be used to determine optimal qMT protocols for reduced B<sub>1</sub>-sensitivity.

**References:** [1] Stikov, n. et al, MRM, doi: 10.1002/mrm.25135 (2014) [2] Boudreau, M. et al, Proc. of ISMRM, #3207 (2014) [3] Boudreau, M. et al, Proc. of ISMRM, #3167 (2014) [4] Sled J. and Pike G. B., JMR, 145:24-36 (2000) [5] Sled J. and Pike G. B., MRM, 46:923-931 (2001) [6] Stikov, N. et al, MRM, 66:725-734 (2011) [7] Harrison, N. et al, Biological Psychiatry, DOI: 10.1016/j.biopsych.2014.09.023 (2014)

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