# Exploring the Design Space of 3D MLLMs for CT Report Generation

Mohammed Baharoon 1,2\*, Jun Ma 1,3,6\*, Congyu Fang 1,3,5, Augustin Toma 1,4, and Bo Wang 1,3,5,6,7  $^{\dagger}$ 

- Vector Institute for Artificial Intelligence, Toronto, Canada
   Department of Biomedical Informatics, Harvard Medical School, Boston, Massachusetts
- <sup>3</sup> Peter Munk Cardiac Centre, University Health Network, Toronto, Canada
  <sup>4</sup> Medical Biophysics, University of Toronto, Toronto, Canada
- Department of Computer Science, University of Toronto, Toronto, Canada
  Department of Laboratory Medicine and Pathobiology, University of Toronto, Toronto, Canada
  - AI Hub, University Health Network, Toronto, Canada
     \* Equal contribution
     † Corresponding Author

Abstract. Multimodal Large Language Models (MLLMs) have emerged as a promising way to automate Radiology Report Generation (RRG). In this work, we systematically investigate the design space of 3D MLLMs, including visual input representation, projectors, Large Language Models (LLMs), and fine-tuning techniques for 3D CT report generation. We also introduce two knowledge-based report augmentation methods that improve performance on the GREEN score by up to 10%, achieving the 2nd place on the MICCAI 2024 AMOS-MM challenge. Our results show that RRG is largely independent of the size of LLMs and freezing the LLMs performs better than fine-tuning or using parameter-efficient techniques. We also show that larger volume size does not always improve performance if the original ViT was pre-trained on a smaller volume size. Lastly, we show that using a segmentation mask along with the CT volume improves performance on RRG. The code will be publicly available to promote future development.

## 1 Introduction

Computed Tomography (CT) is a cornerstone of modern diagnostic imaging, offering detailed insights into internal anatomical structures and playing a critical role in diagnosing a wide range of diseases [7]. However, the rapid increase in the need of CT examinations presents a significant challenge for radiologists, who must interpret complex 3D volumetric data and generate comprehensive reports under tight time constraints [4]. This growing demand places immense pressure on healthcare systems, often leading to delays in diagnosis and treatment, which can adversely affect patient outcomes [24].

To address this challenge, there has been growing interest in developing automated systems using Multimodal Large Language Models (MLLMs) for radiology report generation [31, 3, 2, 28, 8], leveraging their ability to process medical images with advanced natural language generation. A representative example is the Large Language and Vision Assistant (LLaVA) [19], where a vision encoder processes input images, and a projector transforms the encoded features into the language embedding space. These projected embeddings are concatenated with natural language instructions and fed into a language decoder to generate text responses conditioned on both the image and instruction embeddings. LLaVA has been extensively explored for the generation of radiology reports from 2D images [3, 13, 14], with adaptations for the medical domain. For example, MAIRA-2 uses the LLaVA framework for the generation of X-ray reports with localized findings, resulting in more grounded reports [3].

Recent research has expanded to MLLMs for 3D medical images, which offer richer spatial information but introduce computational challenges such as handling volumetric data and managing the high token count [8, 28, 2, 31]. Works, such as M3D [2] and RadFM [28], adopt the LLaVA framework by using a vision-to-language embedding projector. To address the high dimensionality of 3D image embeddings, M3D introduces a spatial pooling layer, while RadFM employs a perceiver module [28].

In this study, we systematically investigate the design space of 3D MLLMs for radiology report generation from CT scans. Our work explores key architectural choices, including visual representation, projectors, LLMs, and fine-tuning strategies. We also introduce heuristic report augmentation methods to improve the completeness of generated reports. The main contributions are summarized as follows:

- **Decoupled architecture design:** we decompose MLLMs into plug-andplay modules, allowing for comprehensive studies to obtain better insights on how these components contribute to performance.
- Knowledge-based argumentation: we introduce two knowledge-based report augmentation methods to enhance report completeness, increasing the performance by over 10%, from 0.366 to 0.470, on the GREEN metric.
- State-of-the-art performance: our solution achieved the 2nd place on the hidden test set of the MICCAI 2024 AMOS-MM challenge.
- Modular implementation: all methods are implemented and open-sourced in a unified framework, ensuring reproducibility, fair comparisons, and easy integration of new methods.

# 2 Methods

In this work, we focus on MLLMs that follow the LLaVA architecture because of their simple yet effective and popular design [19], which includes an image encoder, a projector, and an LLM. Specifically, a Vision Transformer (ViT) [5] is used to extract visual embeddings from an image, followed by a projector to map these embeddings from the image space to the LLM input space, which are then

passed to the LLM as input, along with the query prompt. Next, in Section 2.2, and Section 2.3 we explore different design choices for each element in the MLLM. Lastly, in Section 2.4, we introduce our knowledge-based report augmentation methods, which help to ensure that the final reports are comprehensive.

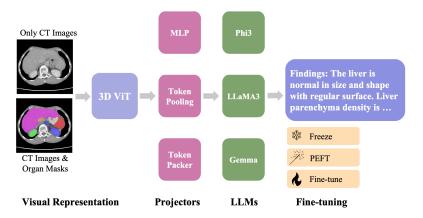


Fig. 1. The design space of 3D MLLMs. We explore different choices in the selection of the visual representation, projectors, LLMs, and fine-tuning methods.

#### 2.1 Visual Representations of 3D Inputs

The major challenge to address in representing 3D volumes for ViTs is the large number of tokens, which leads to a significant computational burden. Different techniques have been developed to reduce token count [17, 2, 28]. AnyResolution [18] has been proposed to embed large image sizes, which divides the high-resolution input into multiple smaller crops, followed by concatenating and compressing their embeddings. We adopt this technique for processing larger 3D CT volumes.

# 2.2 Projector Variants

A naive MLP projector is used as the baseline to project the visual embeddings to the same dimension of LLM input tokens. Spatial pooling perceiver (SPP) projector is the default projector in M3D [2], which reduces the number of tokens while maintaining the 3D spatial structure. TokenPacker [15] reduce the number of tokens by interpolating visual features to low resolution. We extended TokenPacker to take in 3D inputs with one image size by expanding the depth dimension.

## 2.3 Large Language Models and Fine-tuing Methods

We experimented with the instruction-tuned version of Llama 3.1 8B [6], Phi3-mini [1], Qwen 2.5 3B [29], Gemma 2B [23], Mistral 7B [11], and M3D pre-trained LLMs [2]. In addition to freezing the LLMs, we evaluated different fine-tuning techniques: parameter-efficient fine-tuning (PEFT) techniques like LoRA [9] and DoRA [20], and full fine-tuning.

## 2.4 Knowledge-base Report Augmentation

We further augment the generated report to ensure completeness using two introduced methods: Binary-based Questioning (BQ) and naive normality augmentation. Fig 2 shows a graphical representations of the two methods.

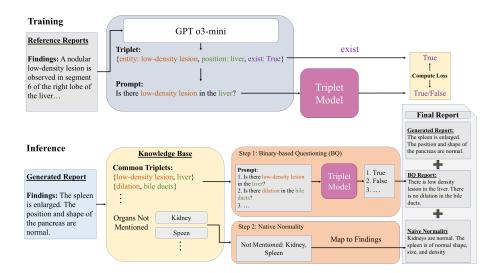


Fig. 2. Knowledge-base report augmentation. After the MLLM generates a report, we apply two additional methods to augment the report, which are Binary-based Questioning (BQ) and naive normality. For BQ, we train a triplet model to answer questions about common conditions and use its answers to append additional findings to the generated report. To train the triplet model, we first prepare a set of question-answer pairs by prompting GPT o3-mini to generate triplets of the entity, location, and existence (in the format {entity, location, exsist}) using findings from the reference reports. These triplets are then reformatted to questions, which are used to prompt the triplet model to generate binary True/False answers based on the CT volume. The value of "exist" is used as ground truth. At inference time, we prompt our triplet model with common triplets, which correspond to common findings, and based on its binary answer we append a positive or negative finding to the report. For naive normality, we append normal findings for organs that are not mentioned in the generated report after the BQ step. These two methods go hand-in-hand to ensure that our reports are complete and do not miss any common findings.

Binary-based Questioning (BQ). In the first part of our report augmentation method, we make additional binary-based question inferencing for common findings on the three regions. Specifically, we first turn reports into triplets with the format {entity, position, exist} following [27]. For example, the finding "A nodular low-density lesion is observed in the right lobe of the liver" becomes {"low-density lesion", "liver", true}. Then, we reformat the triplet into a question in the format "Is there {entity} in the {position}", with the "exist" being the ground truth. If no entity or position is detected, the question format becomes "Is the {position} normal?" or "Can you observe {entity} in this CT scan?", respectively.

The transformation into triplets was done by prompting GPT o3-mini. However, this may result in a lot of variations for the same finding statement (for example, {enlargement, lymph nodes in the retroperitoneum} and {enlargement of lymph nodes, retroperitoneum}). We then prompt GPT o3-mini again to go through all these variations and design a mapping that transforms them all into one common triplet.

We train a model, which we will call the triplet model, to predict the {exist} variable for each triplet, where triplets are constructed from findings in the corresponding report. The triplet model is based on Phi3-mini with an M3D projector, trained for 200 epochs with the same hyperparameters described in Section 3.2. Moreover, we collect the most common triplets and include them as questions in all examples throughout training. For these common triplets, if it, or any of its variations, is already in that CT's findings, we use the associated {exist} variable, otherwise, {exist} is set to false. This ensures that the model is always optimized for answering these common conditions. At inference time, we prompt the model with these common triplets and map its binary answer to pre-defined findings. For example, an answer of "True" for the question "Is there nodules in the lung" would be mapped to "Nodules are seen in the lungs." These questions were designed to be general to improve performance on the metric, but this method can be adapted to specific triplets.

Naive Normality (NN) augmentation. In this method, we predefine a list of organs and conditions along with their associated normality finding for each of the three regions based on common findings from the dataset. Using this list, we then scan through the generated report and add a normality finding to organs or conditions not mentioned in the generated report. For example, in a chest report, we can scan through the generated report to find the word "heart." If it is not mentioned, we add the finding "The heart size and shape is normal and within limits. The heart is normal." to the report. Moreover, in normal findings that require two identifiers, like "No pleural effusion is seen in both pleural cavities or bilateral pleural cavities," we look for both the words "pleural effusion" and "pleural cavities" being in the same sentence.

# 3 Experiments and Results

### 3.1 Dataset

All the experiments are conducted using the MICCAI24 AMOS-MM challenge<sup>8</sup>, originally from the AMOS dataset [10], which includes 1287 and 400 cases for training and validation. We used the validation set as our test set because the test set reports were not released. Each case contains one CT scan and the findings and impressions sections of the associated report for any or all the three regions: chest, abdomen, and pelvis. Chest findings are avaliable in 30.3% of cases, abdomen for 99.8%, and pelvis for 86.9%. We follow the challenge setting and only use the findings as model output. The dataset was gathered from Longgang District Central Hospital and Longgang District People's Hospital in Shenzhen, China.

## 3.2 Implementation details

A 3D ViT pre-trained on Radiopedia, from M3D [2], was used as the image encoder with a patch size of  $4 \times 16^2$  and a volume size of  $32 \times 256^2$ . All MLLMs were trained for 150 epochs using a batch size of 4, with a final learning rate of  $5e^{-5}$  and a cosine scheduler. We used a simple one-sentence prompt instructing the LLM to describe the findings in the CT scan. The Hugging Face Transformers [26] framework was used for all LLM training and inferencing.

For processing larger CT volumes using AnyResolution [18], the volume is divided into crops that are then embedded and concatenated before being passed to the LLM. This allows for handling high-resolution data with ViTs that are pre-trained on lower resolutions, while preserving intricate visual details. We use this method to process CT volumes of dimension  $64 \times 512^2$  using a ViT pre-trained on CTs of size  $32 \times 256^2$ . In addition to the official metric in the competition, GREEN [21], we also computed the RaTEScore [30], and commonly used text similarity metrics such as BLEU, ROUGE, and METEOR [22, 16, 12].

# 3.3 Results

We report medical report generation results for different LLMs, projectors, and fine-tuning methods. We also explore different settings such as volume size, predicting impressions along with findings, and adding segmentation masks. We use the GREEN score [21] as our base evaluation metric, but we also report RaTEScore [30] and text similarity metrics such as BLEU [22], ROGUE [16] and METEOR [12].

**LLMs.** First, we try multiple LLMs of different sizes ranging from 2B to 8B in size to gauge how much the LLM matters for this task. We show our findings in Table 1. Generally, we notice that the task is LLM-independent, for the LLMs we tried, and using a slightly larger LLM or better LLM does not significantly

<sup>&</sup>lt;sup>8</sup> MICCAI 2024 AMOS-MM challenge: https://www.codabench.org/competitions/3137/

| LLM            | Projector | FT Method | GREEN | RaTEScore | BLEU  | ROUGE | METEOR |
|----------------|-----------|-----------|-------|-----------|-------|-------|--------|
| Phi-3 mini     |           |           | 0.366 | 0.573     | 0.272 | 0.384 | 0.357  |
| Gemma 2B       |           |           | 0.359 | 0.572     | 0.274 | 0.392 | 0.365  |
| Llama3.1 8B    | M3D       | Frozen    | 0.359 | 0.570     | 0.264 | 0.379 | 0.355  |
| Qwen2.5 3B     |           | Frozen    | 0.341 | 0.554     | 0.252 | 0.378 | 0.342  |
| Mistralv0.3 7B |           |           | 0.353 | 0.569     | 0.258 | 0.374 | 0.346  |
| M3D Phi-3      |           |           | 0.365 | 0.571     | 0.276 | 0.394 | 0.360  |
| Phi-3 mini     | M3D       |           | 0.366 | 0.573     | 0.272 | 0.384 | 0.357  |
|                | MLP       | Frozen    | 0.346 | 0.563     | 0.268 | 0.386 | 0.359  |
|                | TP        |           | 0.343 | 0.551     | 0.259 | 0.372 | 0.349  |
| Phi-3 mini     | M3D       | Frozen    | 0.366 | 0.573     | 0.272 | 0.384 | 0.357  |
|                |           | LoRA      | 0.336 | 0.549     | 0.253 | 0.361 | 0.343  |
|                |           | DoRA      | 0.321 | 0.546     | 0.251 | 0.360 | 0.343  |
|                |           | FT        | 0.271 | 0.528     | 0.232 | 0.341 | 0.323  |

Table 1. Effects of LLM, projector, and fine-tuning method on the model performance.

increase performance. However, we also notice that Qwen 2.5 performs worse than all the other models, which could be a result of its training data.

**Projector Variants.** We also benchmark different vision-to-text embedding projectors. Our results are shown in Table 1. We notice that the M3D projector [2] outperforms both TokenPacker [15] and the naive MLP projector. This is likely due to the projector's ability to preserve 3D spatial information, compared to the other methods, which confirms the original work's findings [2].

**Fine-tuning Methods.** Moreover, we investigate the effects of using PEFT techniques like LoRA [9] and DoRA [20], compared to full fine-tuning or keeping the LLM frozen. Table 1 shows our results. We notice that, generally, increasing the number of tunable parameters in the LLM correlates negatively with performance, with a frozen LLM performing the best. This could be due to the task's sensitivity to overfitting.

Visual Input Representations. We experiment with increasing the image size and using the AnyResolution method [18]. For AnyResolution, we use a CT volume of size  $64 \times 512^2$ , and process crops of size  $32 \times 256^2$ , resulting in 8 non-overlapping crops being processed in total, per forward pass. We also pass in the original volume resized to  $32 \times 256^2$ , following the original implementation [18]. Table 2 shows our results. Our results show that increasing the image resolution decreases the score across all metrics, on top of the increased computational burden. Going from the  $32 \times 256^2$  image size to  $32 \times 512^2$  increases the number of tokens for the ViT 4 times. This could be due to multiple factors, including the LLMs inability to handle longer contexts and unreliable evaluation metrics.

Additional Experiments. We further experiment with several different training scenarios, such as predicting impressions along with findings and feeding a

**Table 2.** Effect of increasing image resolution. Generally, we observe that increasing the image resolution decreases performance, when the ViT is pre-trained on  $32 \times 256^2$ . Under similar compute, using AnyRes performs better than not.

| Vol. Size           | AnyRes       | GREEN | RaTEScore | BLEU  | ROUGE | METEOR |
|---------------------|--------------|-------|-----------|-------|-------|--------|
| $32 \times 256^2$   | F            | 0.366 | 0.573     | 0.272 | 0.384 | 0.357  |
| $32 \times 512^{2}$ | $\mathbf{F}$ | 0.328 | 0.551     | 0.250 | 0.370 | 0.339  |
| $64 \times 512^2$   | ${ m T}$     | 0.344 | 0.560     | 0.256 | 0.379 | 0.344  |

segmentation mask generated by TotalSegmentor [25], along with the CT volume, where we embed the volume and organ segmentation mask separately and concatenate their embeddings before being passed to the LLM. The results are shown in Table 3. Predicting impressions slightly degrades performance. However, using the segmentation mask along with the volume slightly improves performance on both GREEN and RaTEScore, which could be because it's easier to identify abnormalities and organs with the help of the masks.

**Table 3.** Additional experiments. Predicting the impressions with findings slightly degrades performance, and using the segmentation mask improves performance. Only the findings were used in the evaluation.

| Method            | GREEN | RaTEScore | BLEU  | ROUGE | METEOR |
|-------------------|-------|-----------|-------|-------|--------|
| Baseline          | 0.366 | 0.573     | 0.272 | 0.384 | 0.357  |
| With Impressions  | 0.356 | 0.571     | 0.273 | 0.388 | 0.366  |
| With Segmentation | 0.372 | 0.581     | 0.271 | 0.392 | 0.357  |

Knowledge-base Report Augmentation. Lastly, we report the results for our introduced knowledge-base report augmentation methods. Table 4 shows that both of our methods significantly increase the GREEN score, with naive normality increasing the average score by 8%. We suspect that the disproportionately large increase in the pelvis GREEN is because the reports contain more normal findings. An important observation is that GREEN does not always correlate with the other metrics. Naive normality decreased the score text-similarity metrics and did not have an effect on RaTEScore, which could be indicative of the metric's robustness against these types of tricks.

## 4 Conclusion

Our study reveals that CT report generation with 3D MLLMs is largely LLM-independent, with models from 2B to 8B parameters showing similar performance. The M3D projector outperformed simpler methods by preserving 3D spatial structure, and freezing the LLM, compared to using parameter-efficient techniques or full fine-tuning. Moreover, increasing the input image resolution through the AnyResolution method did not enhance performance, underscoring

**Table 4.** Knowledge-base report augmentation. Both methods significantly increase performance for GREEN. However, naive normality does not affect RaTEScore and decreases text-similarity metrics. Each row builds on the previous one: BQ is added to the baseline, and Naive Normality (NN) is applied on top of BQ.

|          | GREEN |         |                | RaTEScore | BLEU  | ROUGE | METEOR |       |
|----------|-------|---------|----------------|-----------|-------|-------|--------|-------|
| Method   | Chest | Abdomen | ${\bf Pelvis}$ | Avg.      | Avg.  |       | Avg.   |       |
| Baseline | 0.243 | 0.358   | 0.499          | 0.366     | 0.573 | 0.272 | 0.384  | 0.357 |
| + BQ     | 0.260 | 0.391   | 0.526          | 0.392     | 0.599 | 0.264 | 0.410  | 0.384 |
| + NN     | 0.287 | 0.415   | 0.708          | 0.470     | 0.601 | 0.207 | 0.390  | 0.384 |

the need for alignment between the pre-training and fine-tuning image resolutions. Lastly, our introduced knowledge-based report augmentation methods significantly boosted the GREEN score by up to 10%. These insights contribute to a deeper understanding of architectural choices for optimizing automated medical report generation, providing a robust foundation for future research in this domain.

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