Joint Reconstruction of PET-MRI by Parallel Level Sets

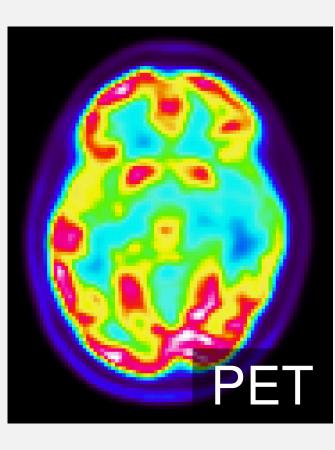
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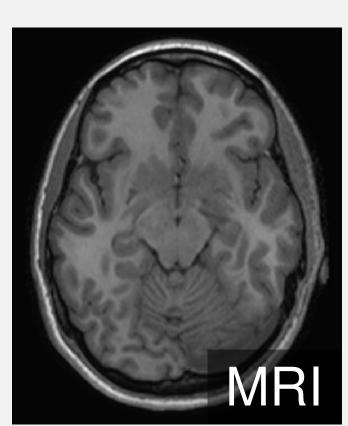
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Motivation: Similar Structures

Combined Positron emission tomography (PET) and magnetic resonance imaging (MRI) scanners acquire functional and anatomical data simultaneously [1]. We aim to exploit the expected similarity during reconstruction.





Method: Parallel Level Sets

We perform joint reconstruction [2] by minimizing

$$\underset{u,v}{\operatorname{argmin}} \|A(u) - f\|^2 + \|B(v) - g\|^2 + \alpha \mathcal{R}(u, v)$$

where the *parallel level sets* functional [3]

$$\mathcal{R}(u,v) := \int \llbracket \nabla u \rrbracket \, \llbracket \nabla v \rrbracket - \llbracket \langle \nabla u, \nabla v \rangle \rrbracket$$

ensures the regularity and structural similarity of the solution. The smoothed norm $[x] := (|x/\beta|^2 + 1)^{1/2}$ regulates which gradients should be taken into account.

This approach was successfully applied to colour image processing [3]. Similar functionals have been used in geophysics [4, 5], colour image processing [6], EIT [7] and multi-modality image registration [8].

Analysis of the Diffusion

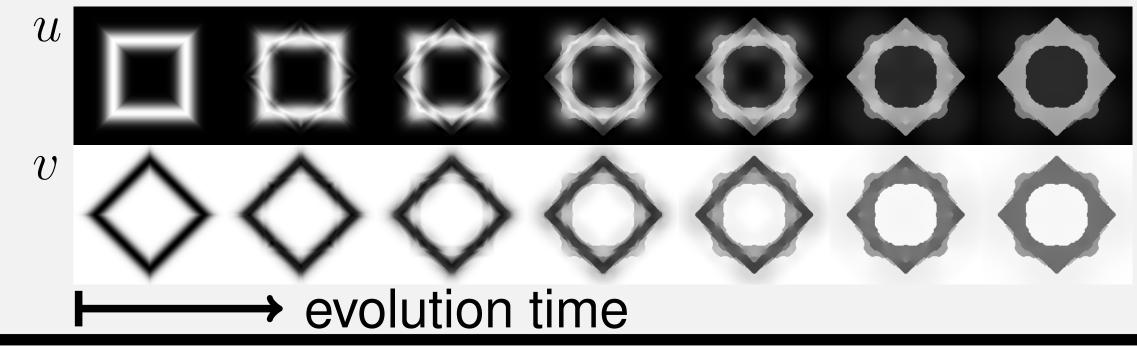
The derivative of $\mathcal R$ with respect to (u,v) takes the form

$$D\mathcal{R}_{u,v} = -\operatorname{div}\left(\frac{K(u,v)\nabla u}{K(v,u)\nabla v}\right)$$

where the diffusivity

$$K(u,v) := \|\nabla v\| \|\nabla u\|^{-1} Id - \|\langle \nabla u, \nabla v \rangle\|^{-1} \nabla v \nabla v^T$$

couples the equations. This results in a flow for u where the principle directions are dictated by v and vice versa. If the edges are aligned there is no flow across the edges. The figure shows the evolution of u and v minimizing the parallel level sets functional.



Conclusions

By coupling two modalities in a joint reconstruction we make use of more information. The images are sharper and of higher quality than separate reconstructions. Errors are greatly decreased in areas of joint edge information.

parallel level sets, error 11.4% parallel level sets, error: 5.6%

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References

[1] D. W. Townsend, "Multimodality Imaging of Structure and Function," Phys Med Biol, vol. 53, no. 4, pp. R1–R39, 2008.

[2] E. Haber and D. W. Oldenburg, "Joint Inversion: A Structural Approach," *Inverse Probl*, vol. 13, pp. 63–77, 1997.

[3] M. J. Ehrhardt and S. R. Arridge, "Vector-Valued Image Processing by Parallel Level Sets," IEEE T Image Process, vol. 23, no. 1, pp. 9–18, 2014.

[4] L. A. Gallardo and M. A. Meju, "Characterization of Heterogeneous Near-Surface Materials by Joint 2D Inversion of DC Resistivity and Seismic Data," *Geophs Res Lett*, vol. 30, no. 13, p. 1658, 2003.

[5] E. Haber and M. Holtzman Gazit, "Model Fusion and Joint Inversion," Surv Geophys, vol. 34, pp. 675–695, 2013.

[6] N. Sochen, R. Kimmel, and R. Malladi, "A General Framework for Low Level Vision," *IEEE T Image Process*, vol. 7, no. 3, pp. 310–318, 1998.

[7] J. P. Kaipio, V. Kolehmainen, M. Vauhkonen, and E. Somersalo, "Inverse Problems with Structural Prior Information," Inverse Probl, vol. 15, pp. 713–729, 1999.

[8] E. Haber and J. Modersitzki, "Intensity Gradient based Registration and Fusion of Multi-Modal Images," in Lect Notes Comput Sc. Berlin Heidelberg: Springer-Verlag, 2006, vol. 46, no. 3, pp. 726–733.





