

# Learning the Sampling for MRI

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Joint work with:

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The Leverhulme Trust



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Physical Sciences  
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# Outline

## 1) Motivation

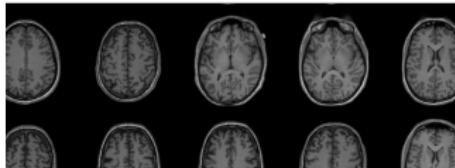


$$\min_x \frac{1}{2} \|SFx - y\|_2^2 + \lambda \mathcal{R}(x)$$

## 2) Bilevel Learning

$$\begin{aligned} & \min_{x,y} f(x,y) \\ & x = \arg \min_z g(z,y) \end{aligned}$$

## 3) Learn sampling pattern in MRI



## Inverse problems

$$A \textcolor{red}{x} = \textcolor{blue}{y}$$

$\textcolor{red}{x}$  : desired solution

$\textcolor{blue}{y}$  : observed data

$A$  : mathematical model

**Goal:** recover  $\textcolor{red}{X}$  given  $\textcolor{blue}{y}$

# Inverse problems

$$A \color{red}{x} = \color{blue}{y}$$

$\color{red}{x}$  : desired solution

$\color{blue}{y}$  : observed data

$A$  : mathematical model

**Goal:** recover  $\color{red}{X}$  given  $\color{blue}{y}$

Hadamard (1902): We call an inverse problem

$A \color{red}{x} = \color{blue}{y}$  **well-posed** if

- (1) a solution  $\color{red}{x}^*$  **exists**
- (2) the solution  $\color{red}{x}^*$  is **unique**
- (3)  $\color{red}{x}^*$  depends **continuously** on data  $\color{blue}{y}$ .

Otherwise, it is called **ill-posed**.



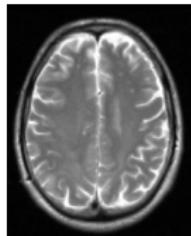
Jacques Hadamard

Most interesting problems are **ill-posed**.

# Example: Magnetic Resonance Imaging (MRI)



MRI scanner

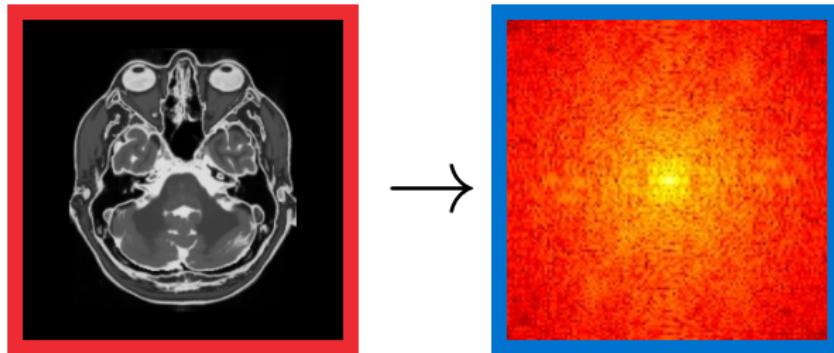


$T_2^*$

**Continuous model:** Fourier transform

$$A\mathbf{x}(s) = \int_{\mathbb{R}^2} \mathbf{x}(s) \exp(-ist) dt$$

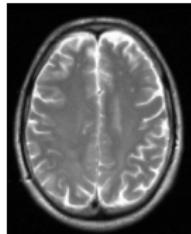
**Discrete model:**  $A = F \in \mathbb{C}^{N \times N}$



# Example: Magnetic Resonance Imaging (MRI)



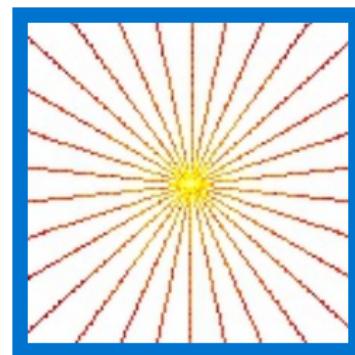
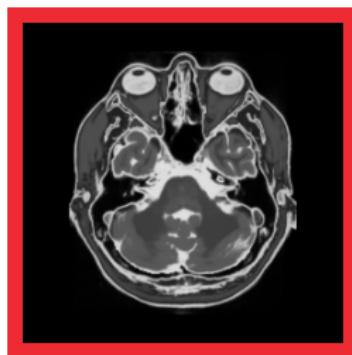
MRI scanner



**Continuous model:** Fourier transform

$$Ax(s) = \int_{\mathbb{R}^2} x(s) \exp(-ist) dt$$

**Discrete model:**  $A = SF \in \mathbb{C}^{n \times N}$



Solution not unique.

# How to solve inverse problems?

## Variational regularization ( $\sim 2000$ )

Approximate a solution  $x^*$  of  $Ax = y$  via

$$\hat{x} \in \arg \min_{x} \left\{ \frac{1}{2} \|Ax - y\|_2^2 + \lambda \mathcal{R}(x) \right\}$$

$\mathcal{R}$  regularizer: penalizes unwanted features, ensures stability and uniqueness

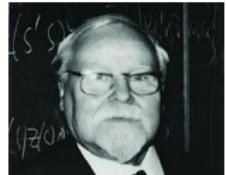
$\lambda$  regularization parameter:  $\lambda \geq 0$ . If  $\lambda = 0$ , then an original solution is recovered. If  $\lambda \rightarrow \infty$ , more and more weight is given to the regularizer  $\mathcal{R}$ .

textbooks: Scherzer et al. 2008, Ito and Jin 2015, Benning and Burger 2018

## Example: Regularizers

**Tikhonov regularization** ( $\sim 1960$ ):

$$\mathcal{R}(\mathbf{x}) = \frac{1}{2} \|\mathbf{x}\|_2^2$$

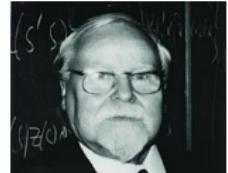


A. Tikhonov

## Example: Regularizers

**Tikhonov regularization** ( $\sim 1960$ ):

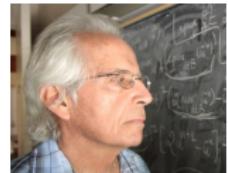
$$\mathcal{R}(x) = \frac{1}{2} \|x\|_2^2$$



A. Tikhonov

**Total Variation** [Rudin, Osher, Fatemi 1992](#)

$$\mathcal{R}(x) = \|\nabla x\|_1$$



S. Osher

$H^1$  ( $\sim 1960\text{-}1990?$ )

$$\mathcal{R}(x) = \frac{1}{2} \|\nabla x\|_2^2$$

**Wavelet sparsity** ( $\sim 1990$ )

$$\mathcal{R}(x) = \|Wx\|_1$$

**Total Generalized Variation:** [Bredies, Kunisch, Pock 2010](#)

$$\mathcal{R}(x) = \inf_v \|\nabla x - v\|_1 + \beta \|\nabla v\|_1$$

# Example: MRI reconstruction

**Compressed Sensing MRI:**

$A = S \circ F$  Lustig, Donoho, Pauly 2007

Fourier transform  $F$ , sampling  $Sw = (w_i)_{i \in \Omega}$

$$\hat{x} \in \arg \min_x \left\{ \frac{1}{2} \|SFx - y\|_2^2 + \lambda \|\nabla x\|_1 \right\}$$



Miki Lustig

# Example: MRI reconstruction

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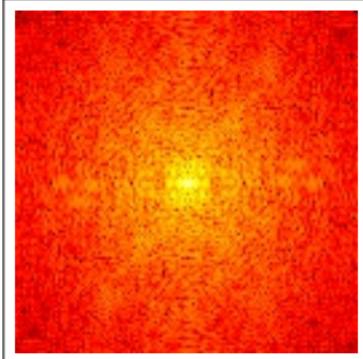
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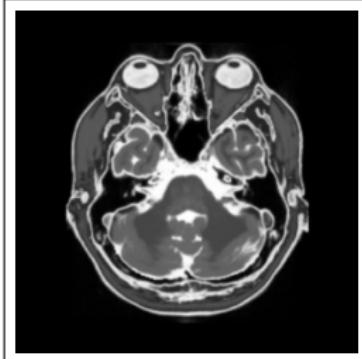
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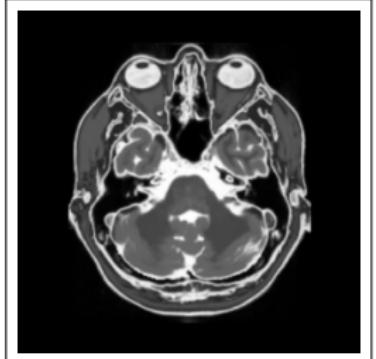
Miki Lustig



sampling  $S^*y$



$\lambda = 0$



$\lambda = 1$

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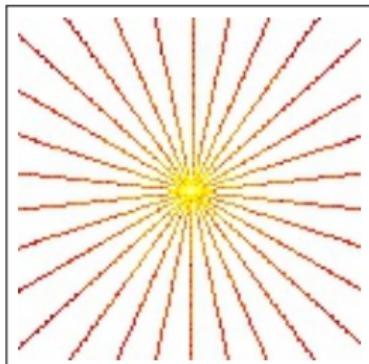
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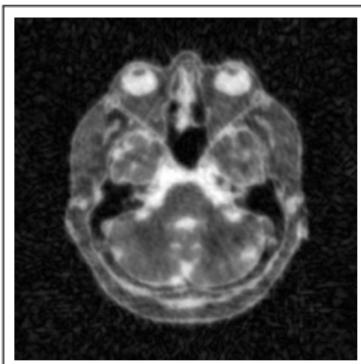
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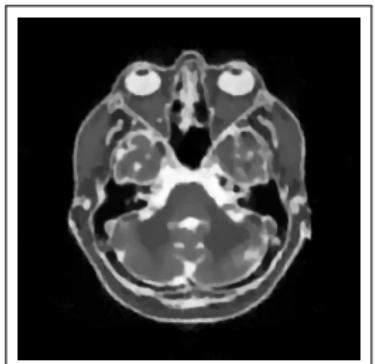
Miki Lustig



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$\lambda = 0$



$\lambda = 10^{-4}$

# Example: MRI reconstruction

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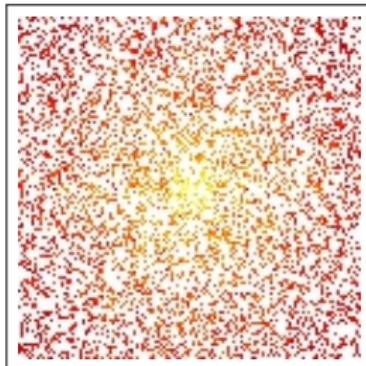
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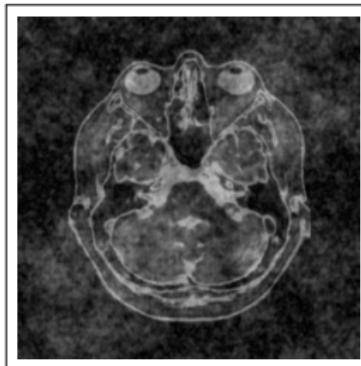
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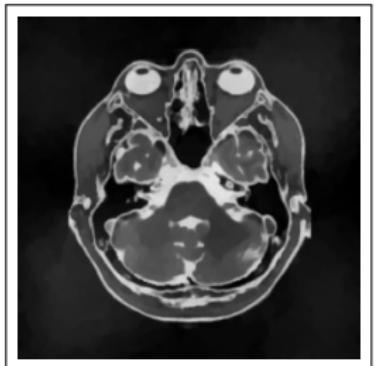
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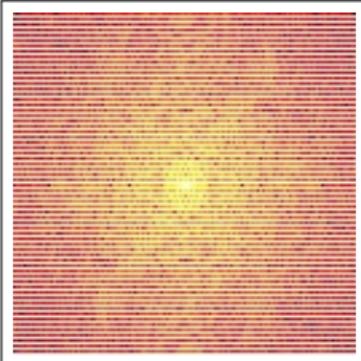
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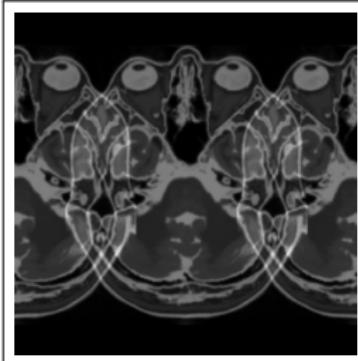
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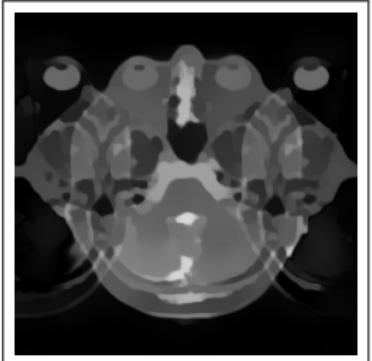
Miki Lustig



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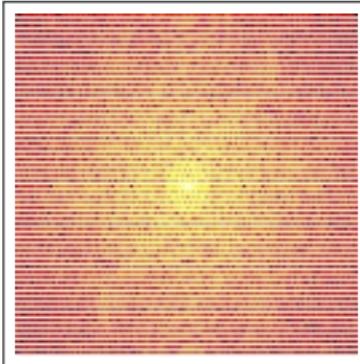
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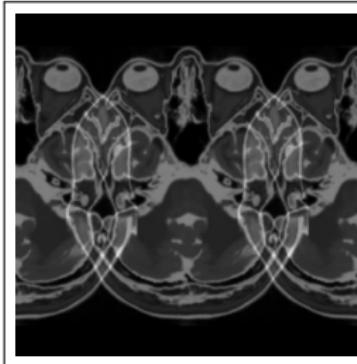
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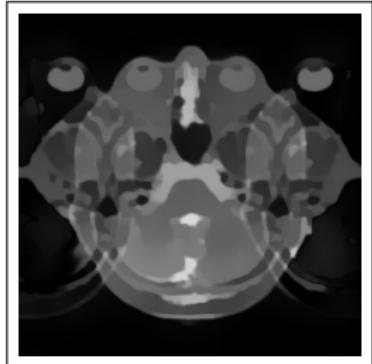
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How to choose the sampling  $S$ ? Is there an optimal sampling?

# Example: MRI reconstruction

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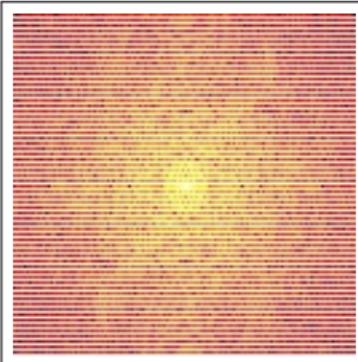
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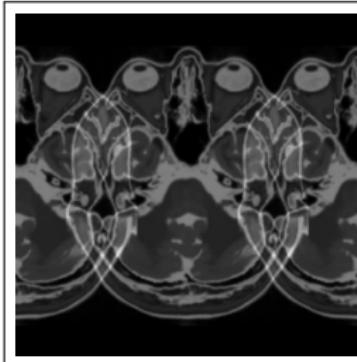
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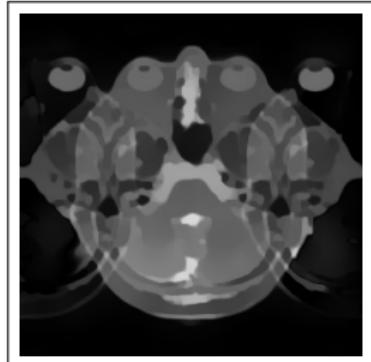
Miki Lustig



sampling  $S^*y$



$\lambda = 0$



$\lambda = 10^{-3}$

How to choose the sampling  $S$ ? Is there an optimal sampling?

Does the optimal sampling depend on  $\mathcal{R}$  and  $\lambda$ ?

# Some important works on sampling for MRI

## Uninformed

- ▶ Cartesian, radial, variable density ... e.g. Lustig et al. 2007
  - ✓ simple to implement
  - ✗ not tailored to application
  - ✗ not tailored to regularizer / reconstruction method
- ▶ compressed sensing **theory**: random sampling, mostly uniform  
e.g. Candes and Romberg 2007
  - ✓ mathematical guarantees
  - ✗ limited to few sparsity promoting regularizers: mostly  $\ell^1$  type
  - ✗ specific yet uninformed class of recoverable signals: sparse

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## Learned

- ▶ **Largest Fourier coefficients** of training set Knoll et al. 2011
  - ✓ simple to implement, computationally light
  - ✗ not tailored to regularizer / reconstruction method
- ▶ **greedy**: iteratively select "best" sample Gözcü et al. 2018
  - ✓ adaptive to dataset, regularizer / reconstruction method
  - ✗ only discrete values, e.g. can't learn regularization parameter
  - ✗ computationally heavy

# Bilevel Learning

## Bilevel learning for inverse problems

$$\hat{x} = \arg \min_x \left\{ \frac{1}{2} \|Ax - y\|_2^2 + \lambda \mathcal{R}(x) \right\}$$

$\mathcal{R}$  smooth and  
strongly convex

# Bilevel learning for inverse problems

**Upper level** (learning):

Given  $(x^\dagger, y), y = Ax^\dagger + \varepsilon$ , solve

$$\min_{\lambda \geq 0, \hat{x}} \|\hat{x} - x^\dagger\|_2^2$$



**Lower level** (solve inverse problem):

$$\hat{x} = \arg \min_x \left\{ \frac{1}{2} \|Ax - y\|_2^2 + \lambda \mathcal{R}(x) \right\}$$

Carola Schönlieb

$\mathcal{R}$  smooth and  
strongly convex

von Stackelberg 1934, Kunisch and Pock 2013, De los Reyes and Schönlieb 2013

# Bilevel learning for inverse problems

**Upper level (learning):**

Given  $(x_i^\dagger, y_i)_{i=1}^n$ ,  $y_i = Ax_i^\dagger + \varepsilon_i$ , solve

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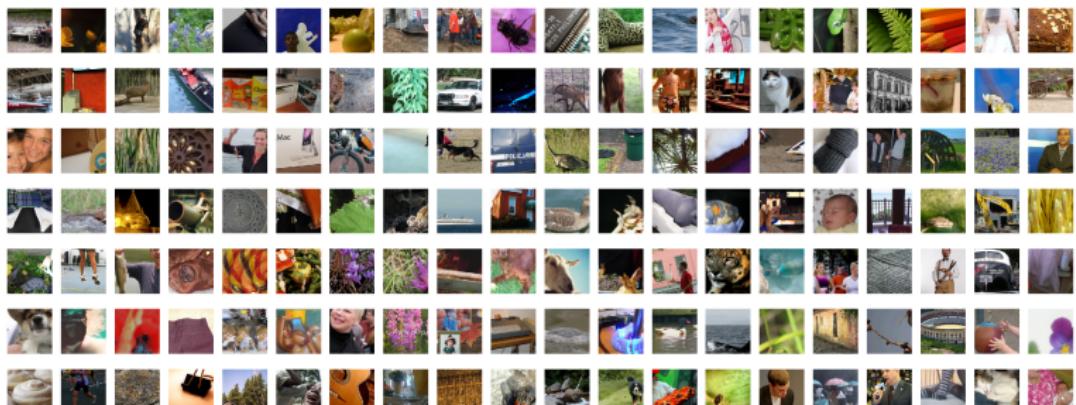
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## Bilevel learning: Reduced formulation

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$$\hat{x} = \arg \min_x L(x, \lambda)$$

# Bilevel learning: Reduced formulation

**Upper level:**

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$$x_\lambda := \hat{x} = \arg \min_x L(x, \lambda)$$

**Reduced formulation:**  $\min_{\lambda \geq 0} U(x_\lambda) =: \tilde{U}(\lambda)$

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$$0 = \partial_x^2 L(x_\lambda, \lambda) \partial_\lambda x_\lambda + \partial_\theta \partial_x L(x_\lambda, \lambda) \quad \Leftrightarrow \quad \partial_\lambda x_\lambda = -B^{-1}A$$

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$$\begin{aligned}\nabla \tilde{U}(\lambda) &= (\partial_\lambda x_\lambda)^* \nabla U(x_\lambda) \\ &= -A^* B^{-1} \nabla U(x_\lambda) = -A^* w\end{aligned}$$

where  $w$  solves  $Bw = \nabla U(x_\lambda)$ .

# Algorithm for Bilevel learning

**Upper level:**  $\min_{\lambda \geq 0, \hat{x}} U(\hat{x})$

**Lower level:**  $x_\lambda := \arg \min_x L(x, \lambda)$

**Reduced formulation:**  $\min_{\lambda \geq 0} U(x_\lambda) =: \tilde{U}(\lambda)$

- ▶ Solve reduced formulation via L-BFGS-B [Nocedal and Wright 2000](#)
- ▶ Compute gradients: Given  $\lambda$ 
  - (1) Compute  $x_\lambda$ , e.g. via PDHG [Chambolle and Pock 2011](#)
  - (2) Solve  $Bw = \nabla U(x_\lambda)$ ,  $B := \partial_x^2 L(x_\lambda, \lambda)$  e.g. via CG
  - (3) Compute  $\nabla \tilde{U}(\lambda) = -A^* w$ ,  $A := \partial_\theta \partial_x L(x_\lambda, \lambda)$

**Learn sampling pattern in MRI**

# Learn sampling pattern in MRI

**Lower level** (MRI reconstruction):

$$R(\lambda, s, y) = \arg \min_x \left\{ \frac{1}{2} \|S(Fx - y)\|_2^2 + \lambda \mathcal{R}(x) \right\}$$

$$S = \text{diag}(s), \quad s_i \in \{0, 1\}$$

Sherry et al. 2019, <https://arxiv.org/pdf/1906.08754.pdf>

# Learn sampling pattern in MRI

**Upper level** (learning):

Given **training data**  $(x_i^\dagger, y_i)_{i=1}^n$ , solve

$$\min_{\lambda \geq 0, s \in \{0,1\}^m} \frac{1}{n} \sum_{i=1}^n \|R(\lambda, s, y_i) - x_i^\dagger\|_2^2$$

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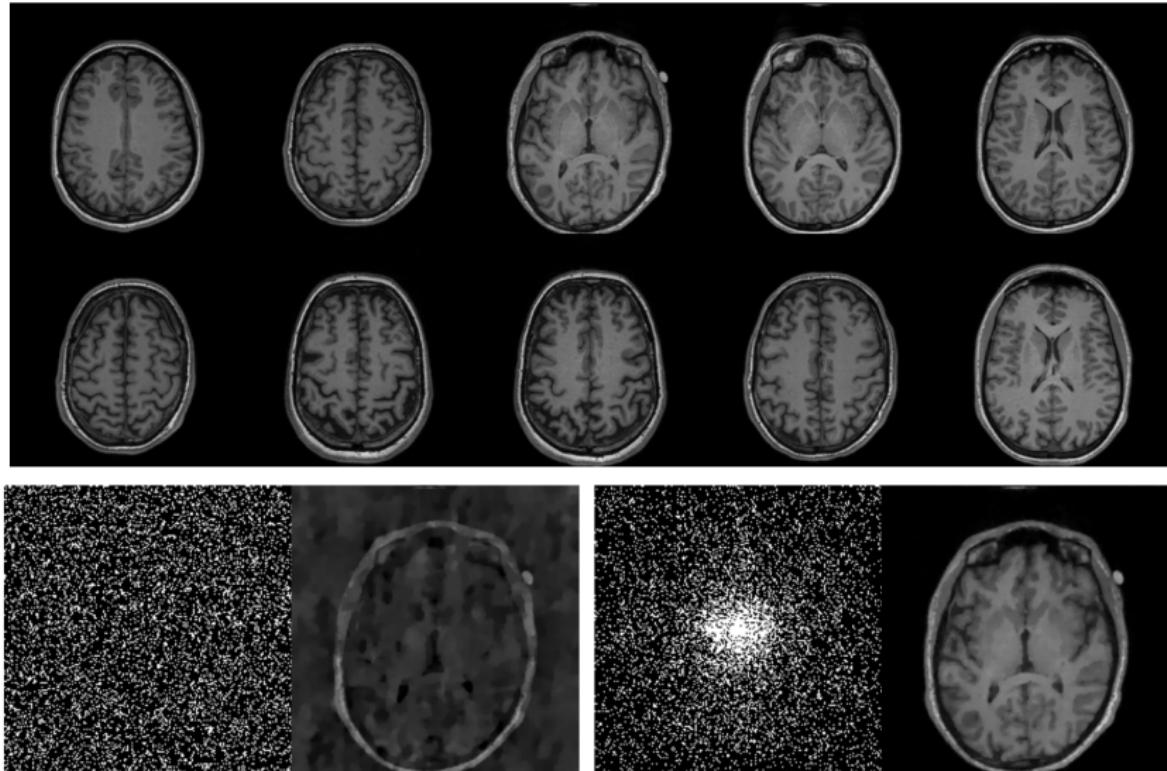
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# Classical compressed sensing versus learned



Uniform random

Reconstruction

Learned

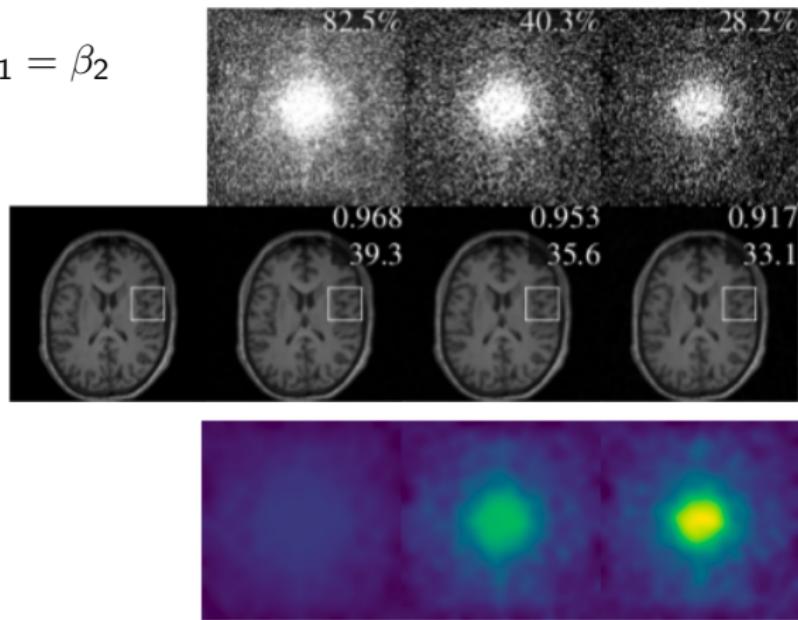
Reconstruction

# Increasing sparsity

Reminder: **Upper level** (learning)

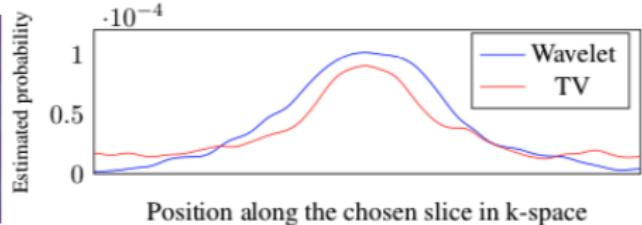
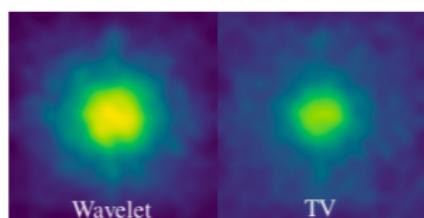
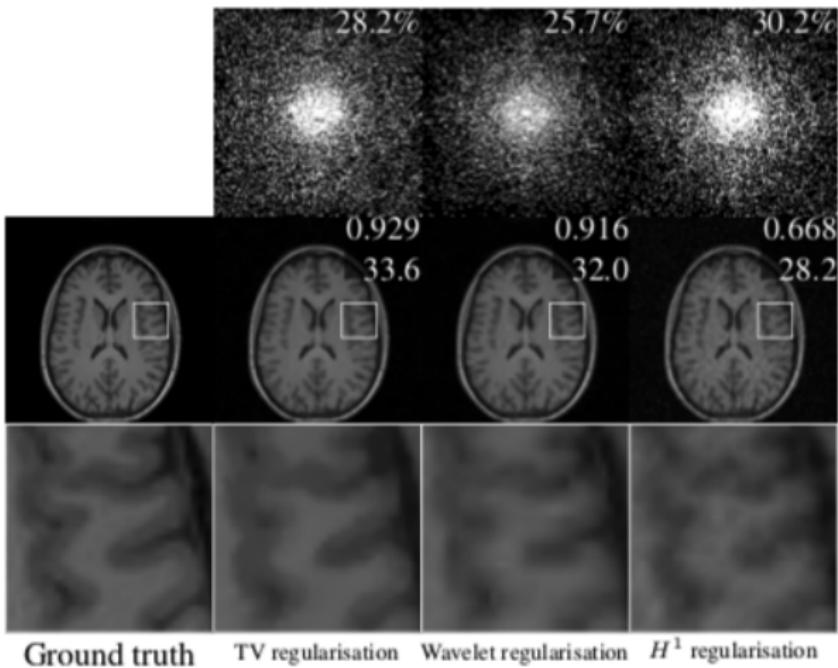
$$\min_{\lambda \geq 0, s \in [0,1]^m} \frac{1}{n} \sum_{i=1}^n \|R(\lambda, s, y_i) - x_i\|_2^2 + \beta_1 \|s\|_1 + \beta_2 \|s(1-s)\|_1$$

$$\beta = \beta_1 = \beta_2$$

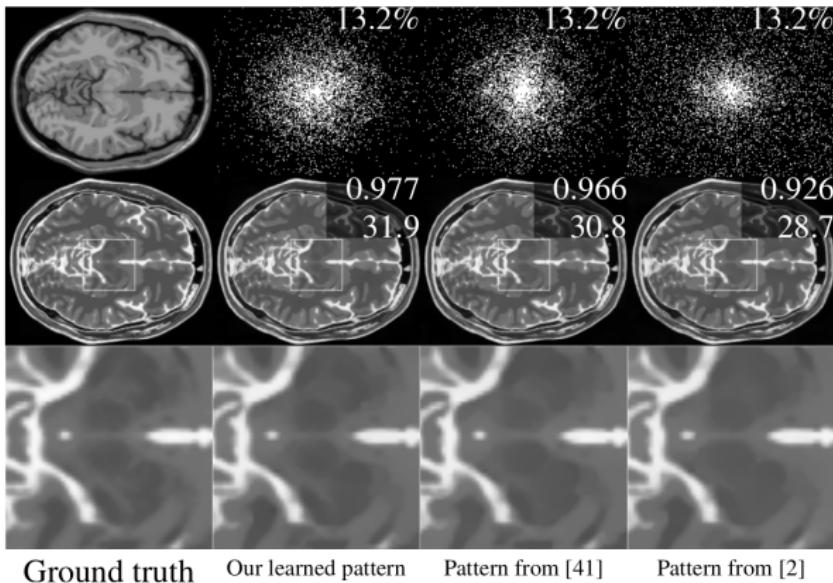


Sherry et al. 2019

# Compare regularizers



# Compare "free" samplings



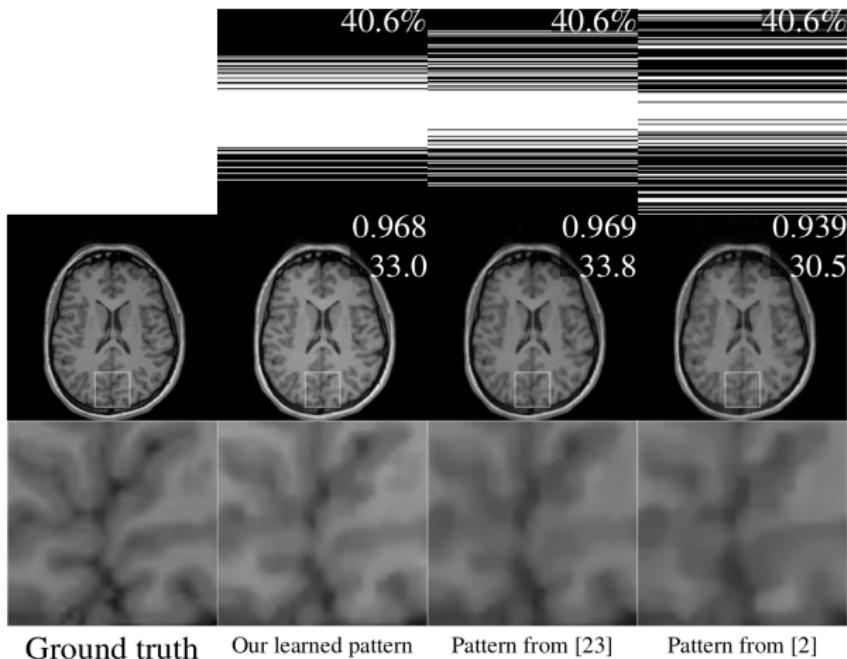
	Pattern type	SSIM	PSNR
Training	Our method	$0.977 \pm 0.002$	$32.5 \pm 0.2$
	Data-adapted [41]	$0.968 \pm 0.002$	$31.1 \pm 0.1$
	Uninformed VDS [2]	$0.925 \pm 0.005$	$28.9 \pm 0.1$
Testing	Our method	$0.975 \pm 0.003$	$32.1 \pm 0.2$
	Data-adapted [41]	$0.967 \pm 0.003$	$31.1 \pm 0.2$
	Uninformed VDS [2]	$0.924 \pm 0.003$	$28.8 \pm 0.1$

"ours" = [Sherry et al. 2019](#)

[41] = [Knoll et al. 2011](#)

[2] = [Lustig et al. 2007](#)

# Compare Cartesian samplings



Ground truth

Our learned pattern

Pattern from [23]

Pattern from [2]

"ours" = Sherry et al. 2019

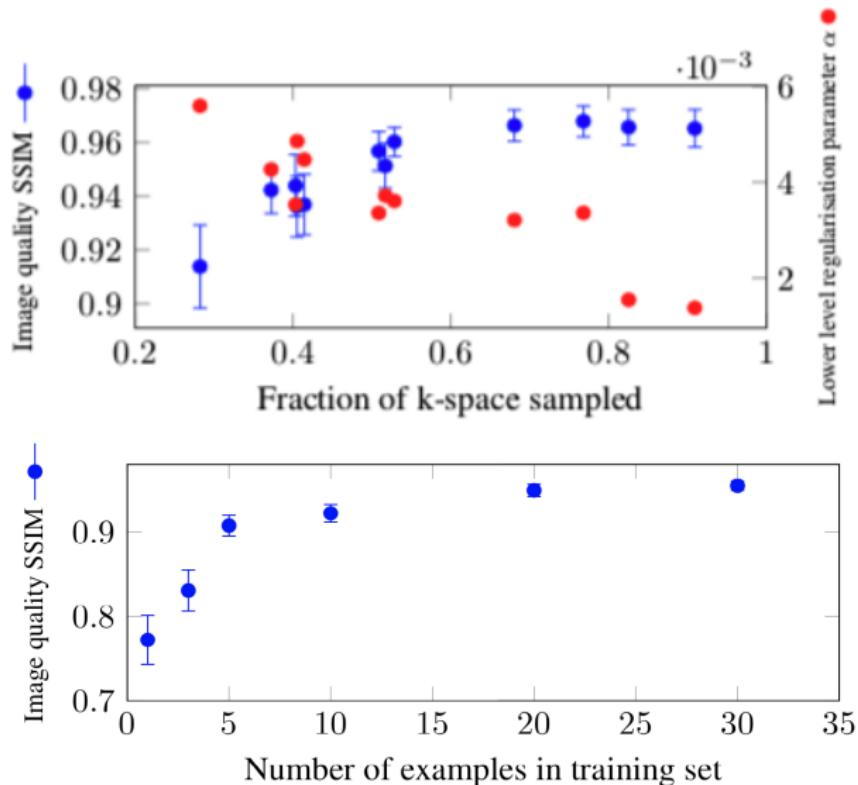
[23] = Gözcü et al. 2018

[2] = Lustig et al. 2007

regularizer = TV

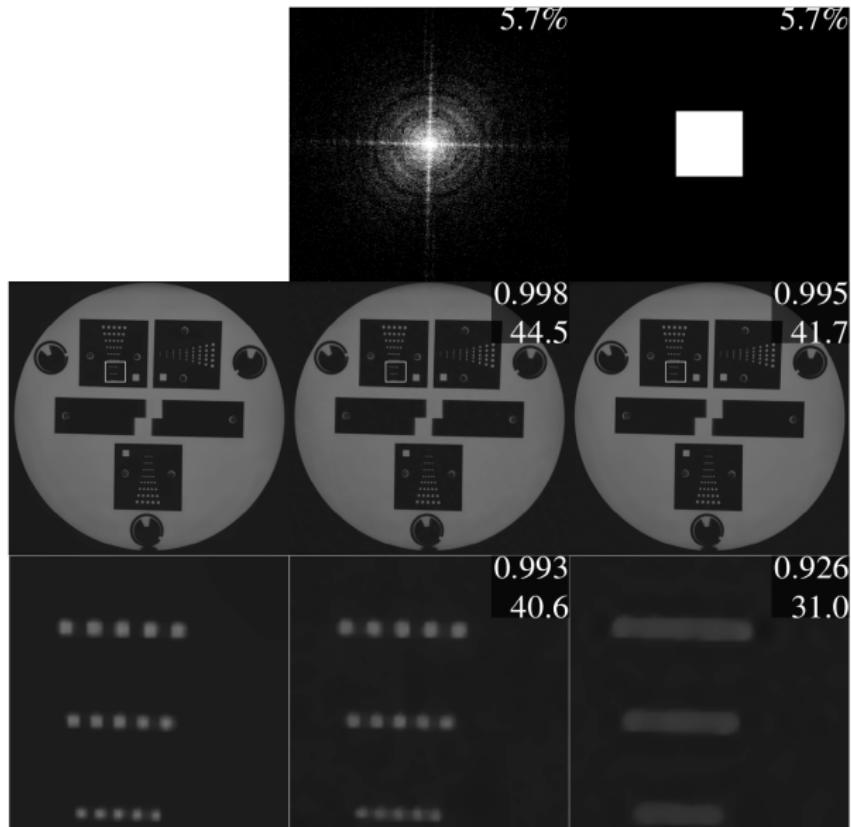
	Line sampling (40.6%)	Free pattern (34.7%)
Our method	4192	6494
The method from [23]	$12087$	$3.90 \cdot 10^8$

## More insights: sampling and number of data



Sherry et al. 2019

# High resolution imaging: $1024^2$



# Conclusions and outlook

## Conclusions

- ▶ Learn parameters via **Bilevel / machine learning**
- ▶ Learned sampling **better** than generic sampling
- ▶ "Optimal" sampling **depends on regularizer**
- ▶ **Very little data** needed

## Outlook

- ▶ Investigate other **algorithms** tailored to problem
  - ▶ DFO with errors in objective (ongoing work with Lindon Roberts)
  - ▶ not based on reduced formulation, e.g. nonlinear ADMM
- ▶ **Unrolling**: replace lower level problem by algorithm
- ▶ **End-to-end learning**: learn reconstruction and sampling