

Easy Perturbation EEG Algorithm for Spectral Importance  
(easyPEASI): A Simple Method to Identify Important Spectral  
Features of EEG in Deep Learning Models

Authors: David Nahmias & Kimberly Kontson (2020)

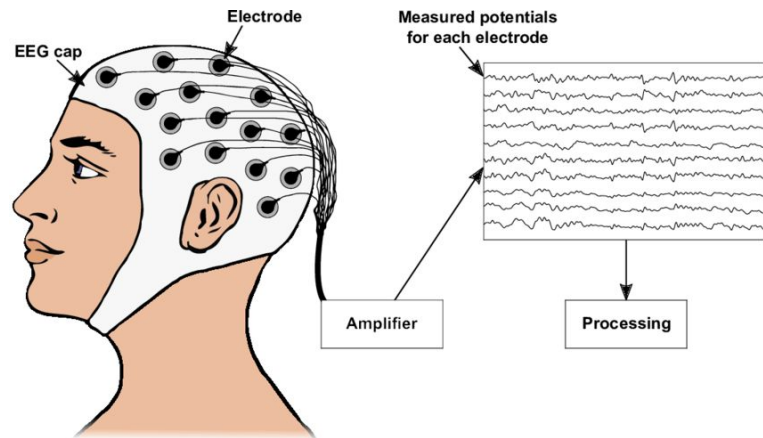
**Trial Lecture by: Mohamed Radwan**

# Agenda

- Discuss core ideas behind the article
- Discuss advantages and flaws in the methods
- Show My attempt to fix those flaws
- Give conclusions of what is the main challenges in the data and reflect what could be possible solutions  
(N.B. My attempts are introducing questions more than answers)

# What is EEG?

- Recording of brain activity which sensors are attached to the scalp to measure electrical signals from the brain by introducing stimuli
- Number of electrodes/channels changes per systems
- Low Signal to Noise ratio (Intrinsic, extrinsic)
- Frequency band:
  - delta (1: 4 Hz),
  - theta (4: 8 Hz)
  - alpha (8: 12 Hz)
  - mu (12: 16 Hz)
  - beta (16: 25 Hz)
  - gamma (25: 40 Hz)



Source: [Sebastian Nagel, 2019](#)

## Frequency Band and Functions

| Brainwave Type              | Frequency Range (Hz) | State of the brain                                     |
|-----------------------------|----------------------|--|
| Delta ( $\delta$ )          | 0.1Hz to 3Hz         | Deep, dreamless sleep, non-REM sleep, unconscious      |
| Theta ( $\theta$ )          | 4Hz to 7Hz           | Intuitive, creative, recall, fantasy, imaginary, dream |
| Alpha ( $\alpha$ )          | 8Hz to 12Hz          | Relaxed, but not drowsy, tranquil, conscious           |
| Low-range Beta ( $\beta$ )  | 12Hz to 15Hz         | Formerly SMR, relaxed yet focused, integrated          |
| Mid-range Beta ( $\beta$ )  | 16Hz to 20Hz         | Thinking, aware of self & surroundings                 |
| High-range Beta ( $\beta$ ) | 21Hz to 30Hz         | Alertness, agitation                                   |
| Gamma ( $\gamma$ )          | 30Hz to 100+Hz       | Motor Functions, higher mental activity                |

Source: [Sugumar Durai and P. T. Vanathi, 2017](#)

# Background and Motivation

- Deep Learning models can achieve state of the art results but it lacks clarity and interpretability.
- Interpretability is critical in medical research
- There are several approaches to measure the effects of features on the prediction of the models
- In Machine Learning, feature importance is done by corrupting one feature and check how the model performs.
- Adding noise to the features is one way (i.e. perturbation)

## Objective of the article

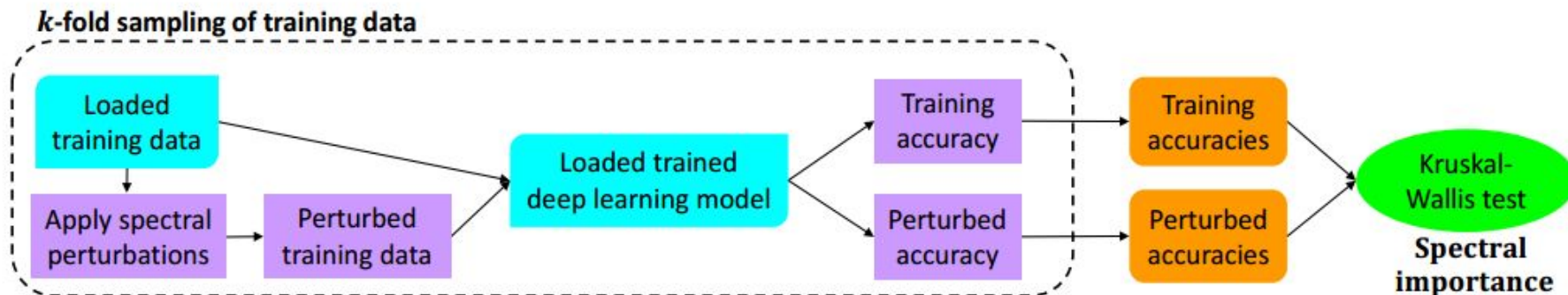
- Determining which frequency band is important for the model to make predictions
- This is done by adding random noise to each one feature at a time
- First Task: Binary classification of each EEG into normal/abnormal
- Second Task: Binary classification of each EEG into for identification of medications

## Used Data

- Released by Temple University Hospital (TUH) Neural Engineering Data Consortium (NEDC)
- EEG Corpus 35,370 EEGs spanning the years from 2002 to present. (1.1TB) from approximately 13,486 subjects
- Each record has a report containing clinical impressions and patient characteristics, including age and sex and medications
- Data is annotated as normal/abnormal
- Each sample consists of (#channels, #time steps)
- Reference: <https://isip.piconepress.com/>

# Methods

- Train binary classification models on the original data (10 models using KFold)
- Perturb one feature at a time from the original data and check the model performance
- Run Kruskal Wallis test to see if there are significant changes in accuracies



Source: [David Nahmias and Kimberly Kontson, 2020](#)



# Algorithm

Source: [David Nahmias and Kimberly Kontson, 2020](#)

**Algorithm** easyPEASI: Easy perturbation EEG algorithm for spectral importance

---

```
1: function PERTURBEEGBANDS(EEG,F_Low,F_High)
2:   for channel  $\in$  EEG do
3:      $\Omega \leftarrow rFFT(EEG[channel])$ 
4:      $\mu \leftarrow Mean(\Omega[F\_Low,F\_High])$ 
5:      $\sigma \leftarrow SD(\Omega[F\_Low,F\_High])$ 
6:      $\Omega[F\_Low,F\_High] \leftarrow \mathcal{N}(\mu, \sigma)$ 
7:      $EEG[channel] \leftarrow irFFT(\Omega)$ 
8:   return EEG

1: function BANDIMPORTANCE(k,F_Low,F_High)
2:   for i  $\leftarrow$  0 to k - 1 do
3:     EEG, Labels  $\leftarrow LoadTrainData(i)$ 
4:     Model  $\leftarrow LoadTrainedDeepModel(i)$ 
5:     PerturbedEEG  $\leftarrow PerturbEEGBands(EEG,F\_Low,F\_High)$ 
6:     TrainAcc[i]  $\leftarrow EvalModel(Model,EEG,Labels)$ 
7:     PerturbAcc[i]  $\leftarrow EvalModel(Model,PerturbedEEG,Labels)$ 

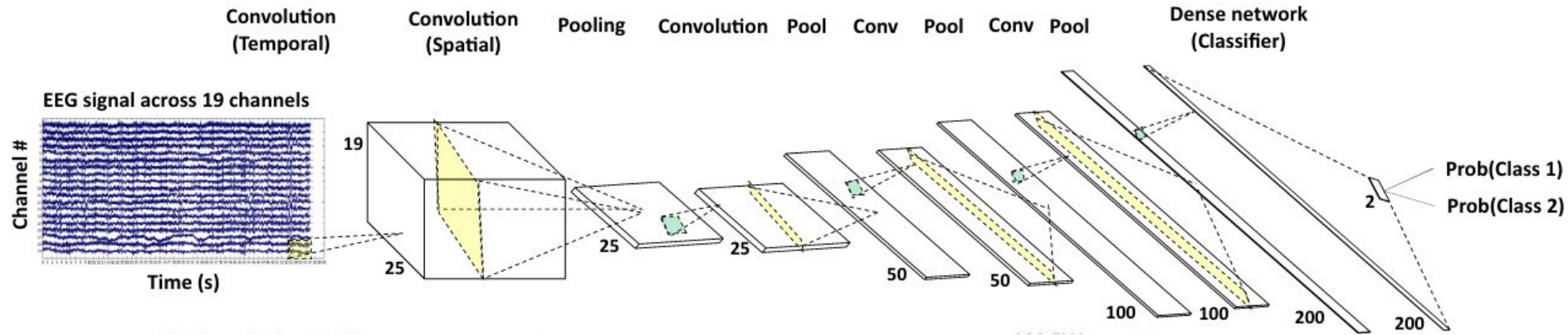
8:    $P \leftarrow KruskalWallisTest(TrainAcc,PerturbAcc)$ 
9:    $\Delta \leftarrow ||Mean(TrainAcc) - Mean(PerturbAcc)||$ 
10:  return P,  $\Delta$ 

1: procedure EASYPEASI( )
2:   k  $\leftarrow$  10  $\triangleright$  k-fold samplings
3:   BandFreqLim  $\leftarrow$  [1,4,8,16,25,40]  $\triangleright$  Hz
4:   for b  $\leftarrow$  0 to length(BandFreqLim)-2 do
5:     F_Low  $\leftarrow$  BandFreqLim[b]
6:     F_High  $\leftarrow$  BandFreqLim[b+1]
7:     P,  $\Delta \leftarrow BandImportance(k,F\_Low,F\_High)$   $\triangleright$  Results
```

---

# Used Neural Networks (DCNN)

- Traditional CNN with convolution and pooling layers



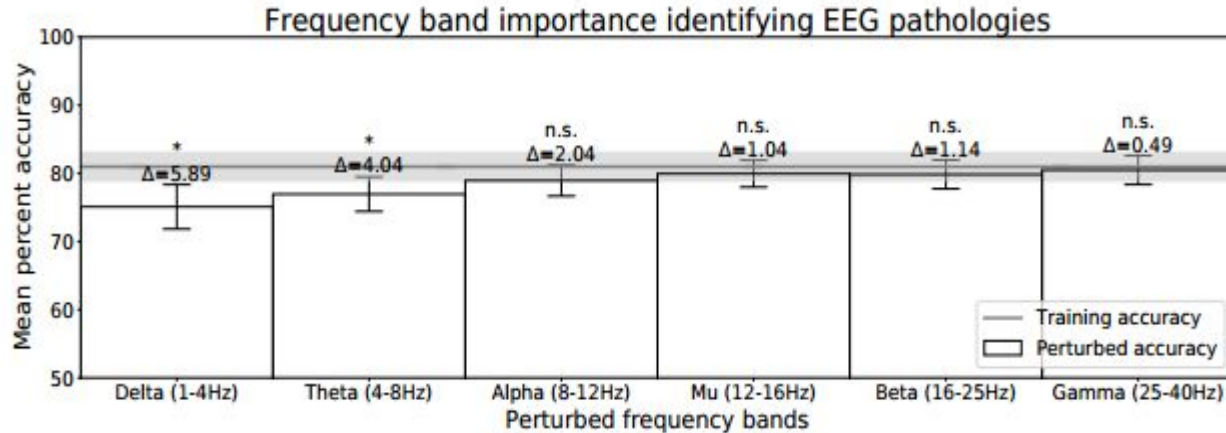
Source: [David Nahmias, Eugene Civillico and Kimberly Kontson, 2020](#)

## Accuracy of identifying EEG pathologies

| <b>Classification</b>          | <b><i>n</i>-train<br/>(<i>n</i>-test)</b> | <b>Train accuracy (%)<br/>(Test accuracy (%))</b> |
|--------------------------------|---|---|
| Normal EEG vs.<br>Abnormal EEG | 10,802<br>(1,200)                         | 80.99 ± 2.22<br>(80.40 ± 2.41)                    |

Source: [David Nahmias and Kimberly Kontson, 2020](#)

# Frequency bands for identifying EEG pathologies



Source: [David Nahmias and Kimberly Kontson, 2020](#)

# Accuracy of identifying medications

| <b>Classification</b>                    | <b><i>n</i>-train<br/>(<i>n</i>-test)</b> | <b>Train accuracy (%)<br/>(Test accuracy (%))</b> |
|--|---|---|
| Dilantin vs. Keppra<br>with Normal EEG   | 316<br>(34)                               | 80.19 ± 13.86<br>(59.12 ± 7.49)                   |
| Dilantin vs. Keppra<br>with Abnormal EEG | 476<br>(52)                               | 83.91 ± 3.48<br>(60.39 ± 5.03)                    |

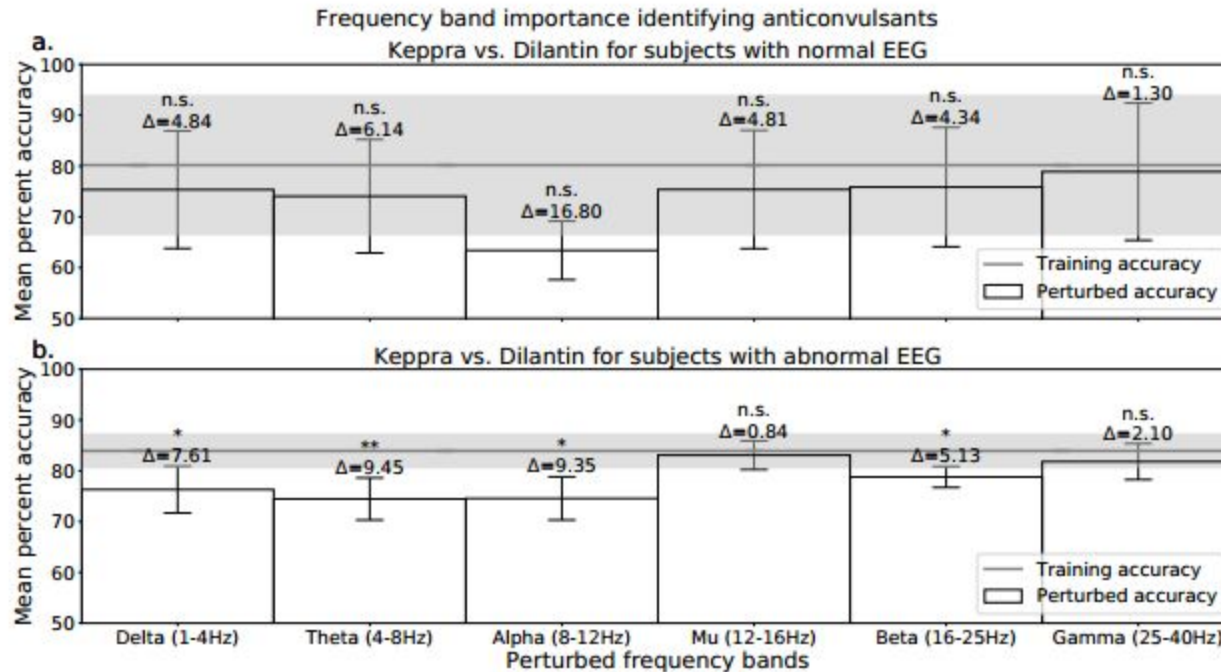
Source: [David Nahmias and Kimberly Kontson, 2020](#)

## Identifying medications (From subsequent study by same authors)

| Classification                                      | n-total (n-test) | Feature-based methods         |                                      |                                     | Network-based methods      |                               |                                      |                            |
|---|------------------|-------------------------------|--------------------------------------|-------------------------------------|----------------------------|-------------------------------|--------------------------------------|----------------------------|
|   |                  | SVM %<br>(P-value)            | kSVM %<br>(P-value)                  | RF %<br>(P-value)                   | LNN %<br>(P-value)         | SCNN %<br>(P-value)           | DCNN %<br>(P-value)                  | EEGNet %<br>(P-value)      |
| Dilantin vs. Kep-<br>pra with Normal<br>EEG         | 350 (34)         | 51.18 ± 6.47<br>(P < .939)    | 58.23 ± 5.23 *<br>(P < .004)         | <b>58.53 ± 4.25</b><br>(P < .013)   | 51.47 ± 7.70<br>(P < .699) | 53.24 ± 7.94<br>(P < .117)    | 55.59 ± 8.77<br>(P < .466)           | 49.12 ± 8.63<br>(P < .074) |
| Dilantin vs. Kep-<br>pra with Abnormal<br>EEG       | 528 (52)         | 57.50 ± 3.69 *<br>(P < .009)  | 57.88 ± 5.99 *<br>(P < .009)         | <b>64.23 ± 6.58 *</b><br>(P < .006) | 50.77 ± 6.09<br>(P < .704) | 56.35 ± 6.02 *<br>(P < .003)  | 60.19 ± 4.94<br>(P < .046)           | 39.42 ± 8.21<br>(P < .062) |
| Dilantin vs. No<br>medications with<br>Normal EEG   | 358 (34)         | 58.61 ± 5.75 *<br>(P < .004)  | 59.17 ± 6.34<br>(P < .011)           | 61.94 ± 6.58 *<br>(P < .006)        | 47.94 ± 8.43<br>(P < .877) | 60.00 ± 7.69 *<br>(P < .008)  | <b>66.76 ± 6.58 **</b><br>(P < .001) | 54.12 ± 5.61<br>(P < .378) |
| Dilantin vs. No<br>medications with<br>Abnormal EEG | 640 (64)         | 66.72 ± 6.78 **<br>(P < .001) | <b>70.78 ± 3.28 **</b><br>(P < .001) | 70.00 ± 2.95 **<br>(P < .001)       | 52.66 ± 3.05<br>(P < .638) | 64.53 ± 5.68 **<br>(P < .001) | 68.59 ± 6.11 **<br>(P < .001)        | 45.00 ± 3.81<br>(P < .493) |
| Keppra vs. No<br>medications with<br>Normal EEG     | 350 (34)         | 55.59 ± 4.45<br>(P < .023)    | 56.47 ± 8.50<br>(P < .120)           | 57.65 ± 7.69<br>(P < .339)          | 51.18 ± 6.20<br>(P < .702) | 55.88 ± 6.44<br>(P < .065)    | <b>62.94 ± 6.34 **</b><br>(P < .001) | 49.12 ± 8.22<br>(P < .646) |
| Keppra vs. No<br>medications with<br>Abnormal EEG   | 528 (52)         | 71.54 ± 5.76 **<br>(P < .001) | <b>73.46 ± 3.92 **</b><br>(P < .001) | 70.00 ± 4.80 **<br>(P < .001)       | 48.84 ± 5.17<br>(P < .820) | 70.77 ± 3.42 **<br>(P < .001) | 68.65 ± 6.66 **<br>(P < .001)        | 51.92 ± 7.60<br>(P < .704) |

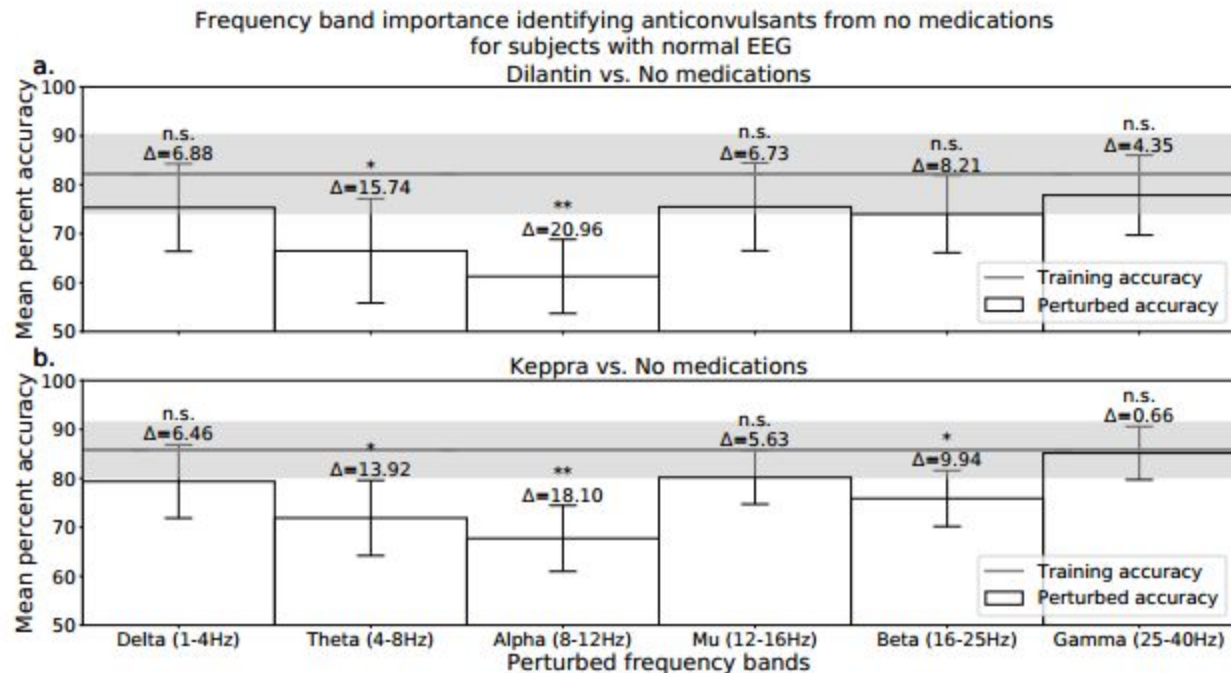
Source: [David Nahmias, Eugene Civillico, Kimberly Kontson, 2020](#)

# Frequency bands for identifying medications (Keppra vs Dilantin)



Source: [David Nahmias and Kimberly Kontson, 2020](#)

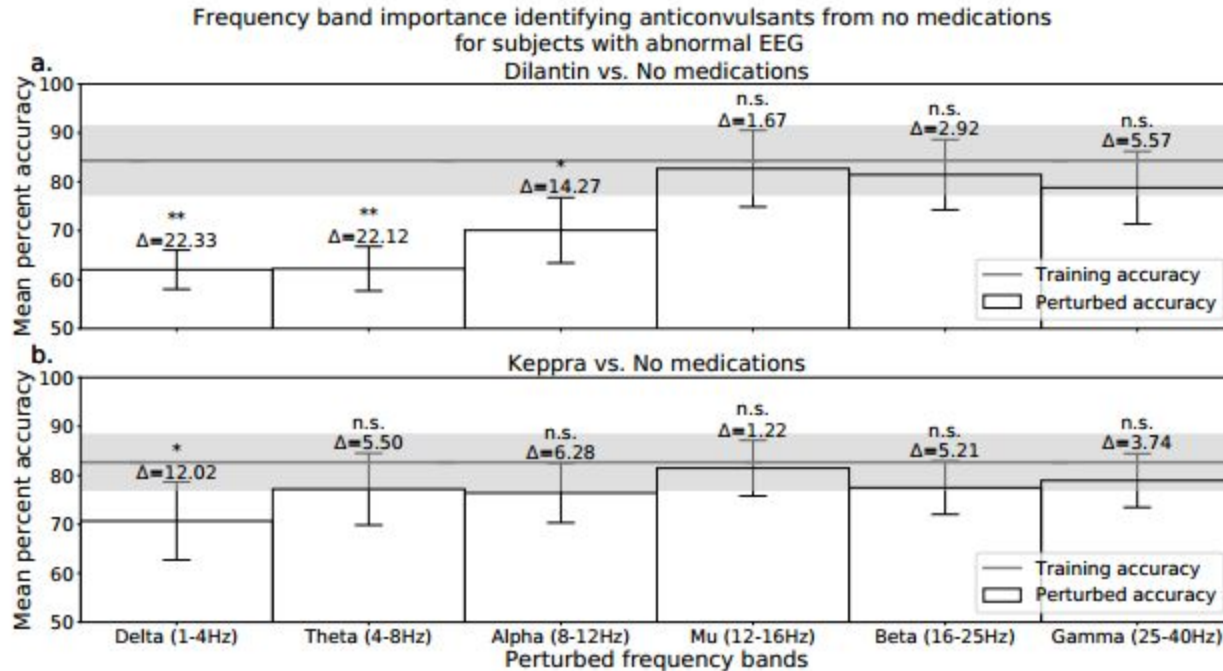
# Frequency bands for identifying medications (medications vs no medications for normal pathology)



Source: [David Nahmias and Kimberly Kontson, 2020](#)



# Frequency bands for identifying medications (medication vs no medication for abnormal pathology)



# Advantages

- The methods are simple and straightforward: The authors combined several simple building blocks to make a novel methods
- The methods follow the standard workflow of machine learning in terms of train test split, KFold cross validation and handling imbalanced data (but with a few flaws).

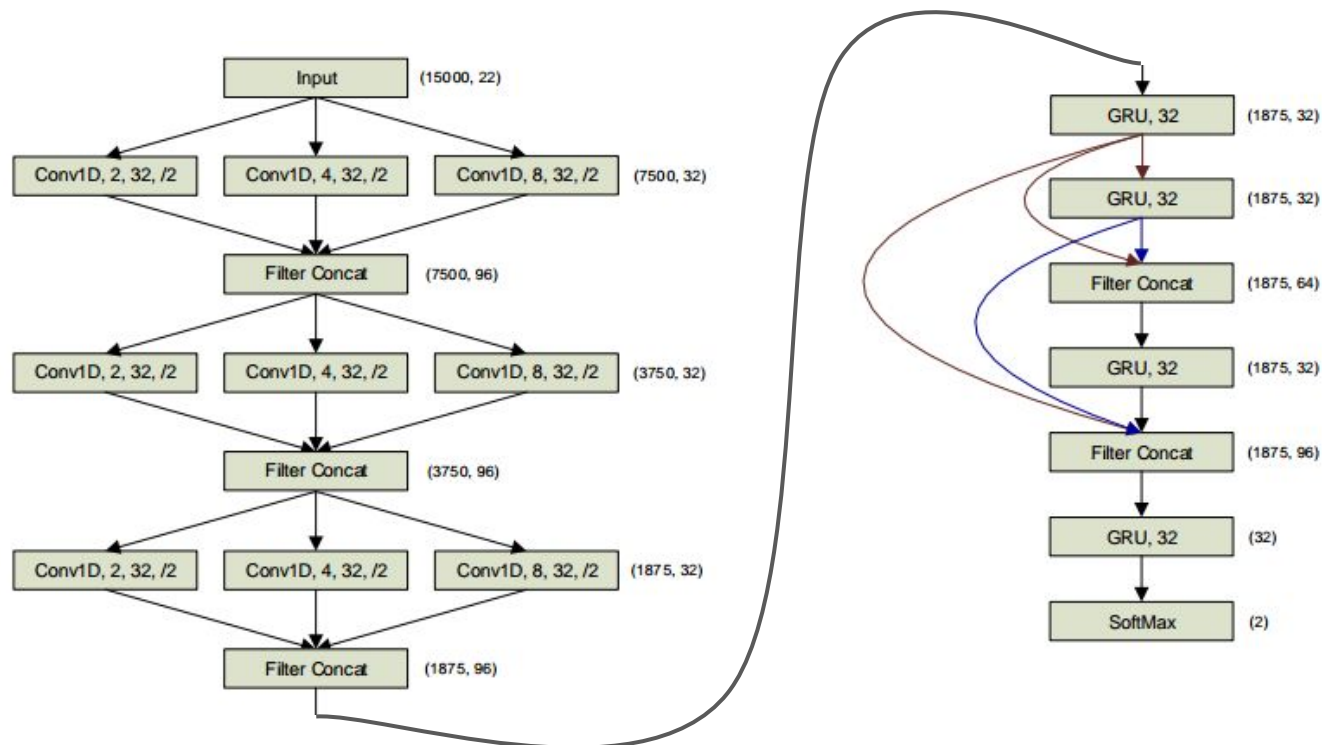
# Flaws

- The authors used training accuracies for comparisons ?
- The data is HUGE which makes almost any model will work and give acceptable accuracies. This means that the model will not generalize to different smaller set of data.

# My Work

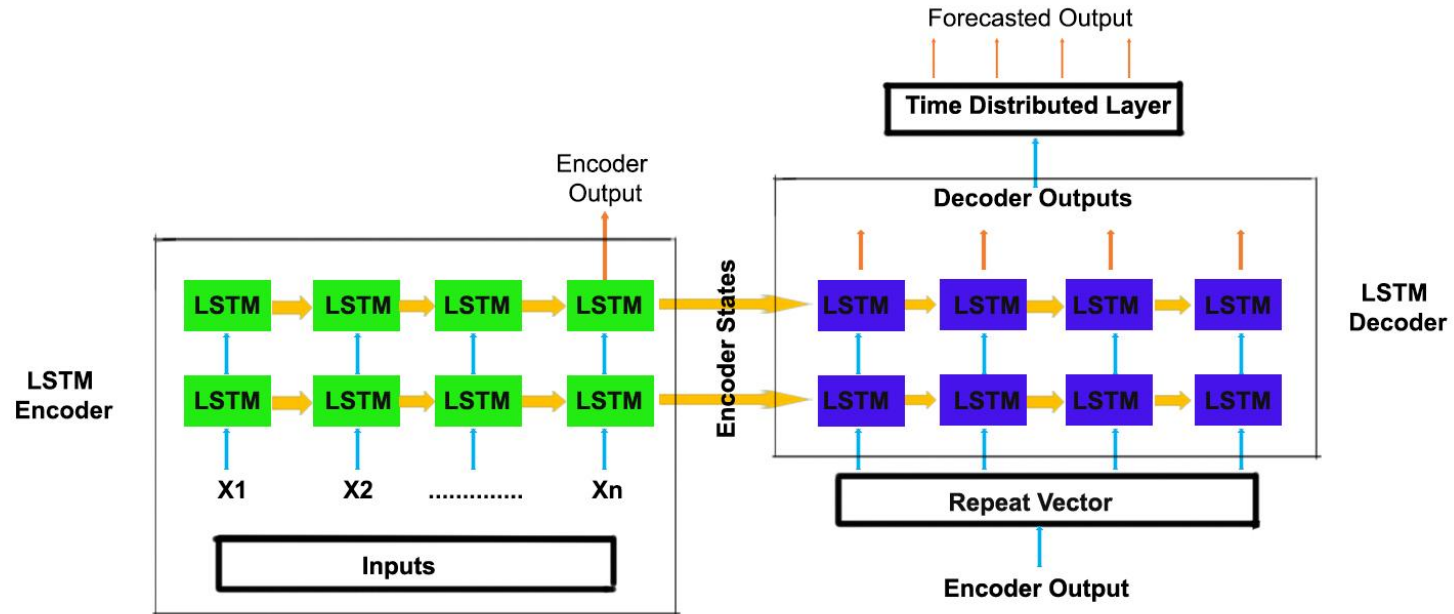
- 1.1TB is not possible to download or saving on disk or using for training using my resources (35,370 EEGs)
- Instead, we use small subset of the data (560 EEGs which is only 12GB).
- Similar workflow was used in terms of data preprocessing
- Some modifications have been made to the workflow
- Tried different models for training instead of DCNN ([Using DCNN leads to instability in performance](#))
- Main Models: [DCNN](#), [LSTM](#), [LSTM Autoencoder](#), [ChronoNet](#)
- [Data Augmentation](#) such as: [filtering](#) and [noising](#).

# ChronoNet



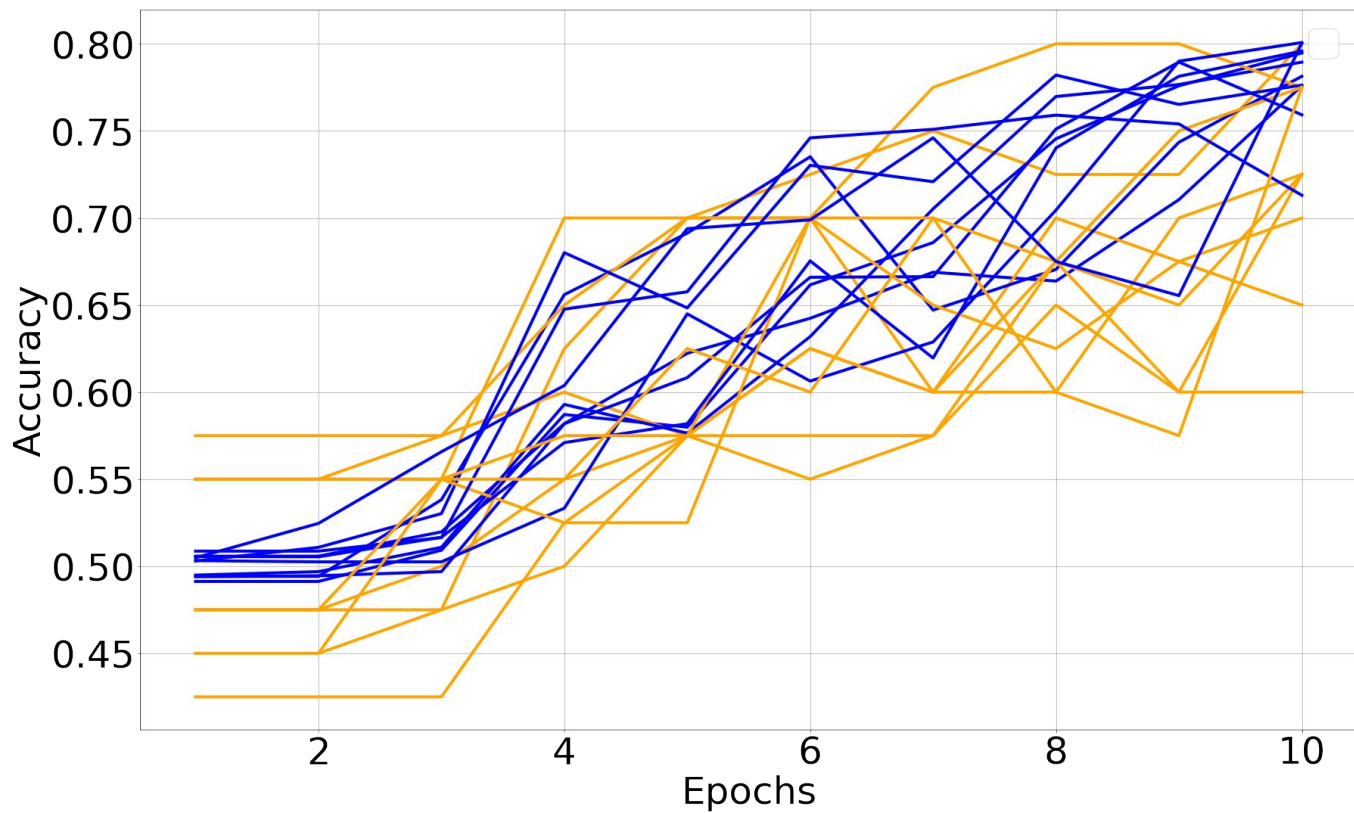
Source: [Subhrajit Roy, et al., 2018](#)

# LSTM Autoencoder

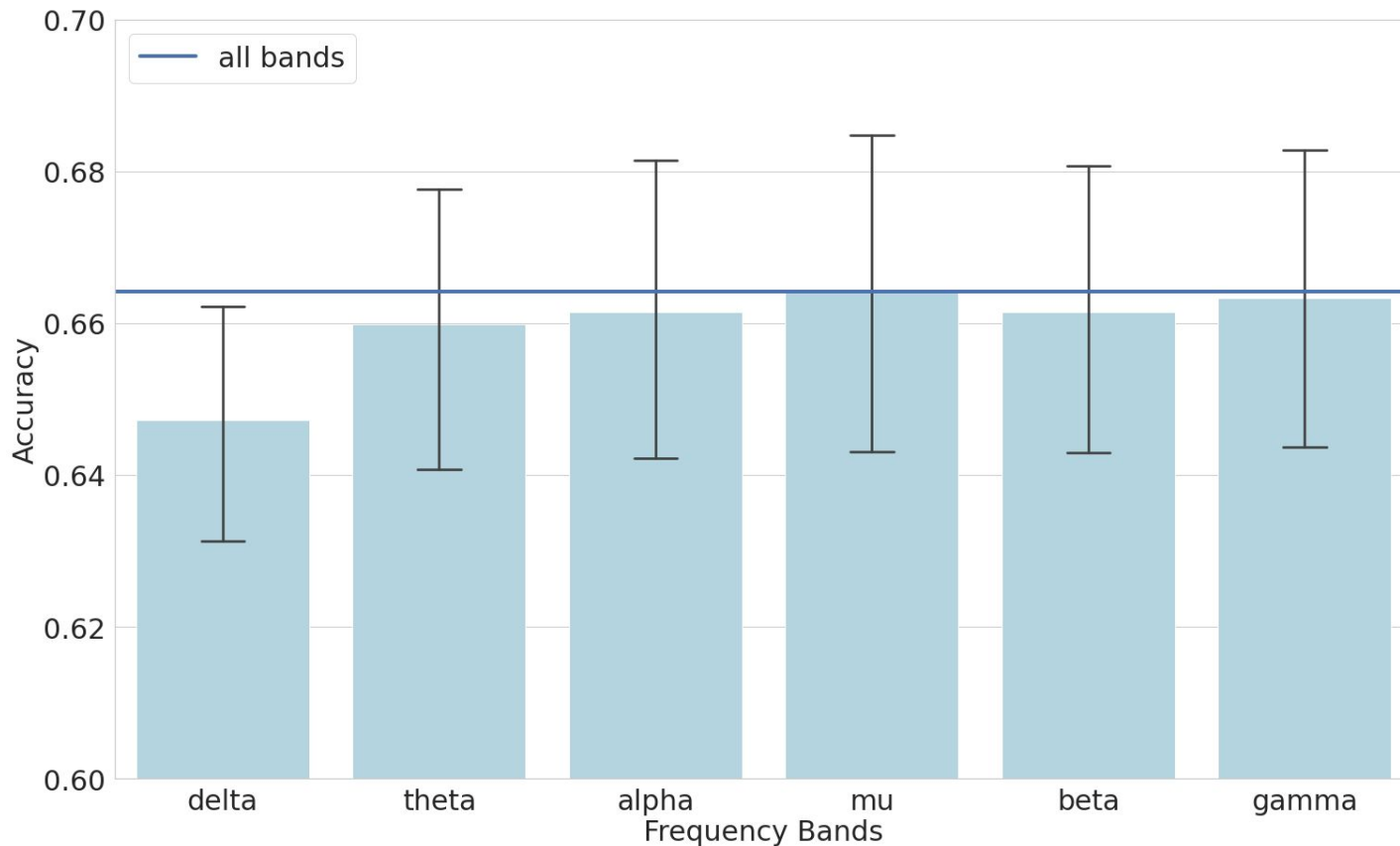


Source: [www.analyticsvidhya.com](http://www.analyticsvidhya.com)

## Results: KFold Validation Curve for identifying EEG pathologies

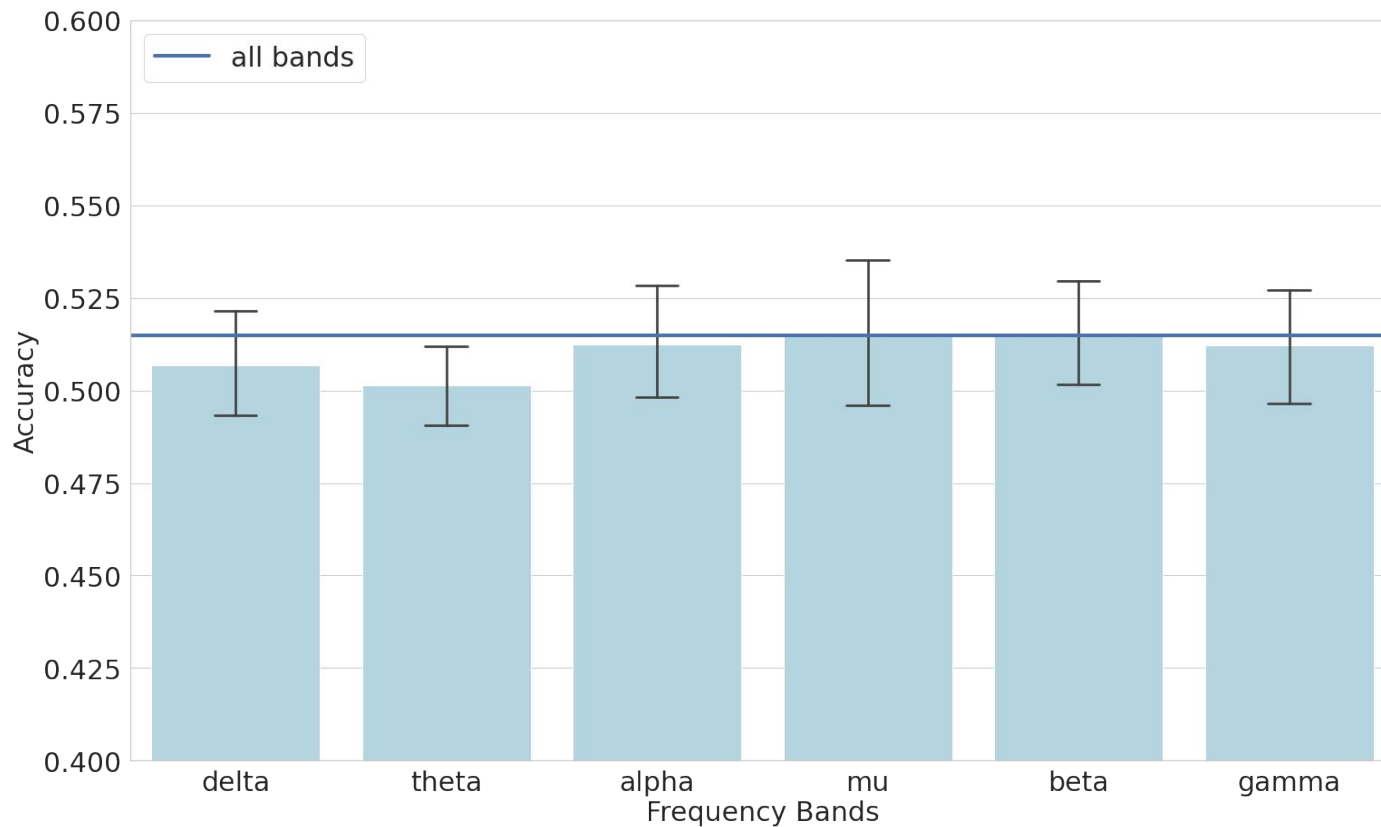


# Results: Frequency band importance (Identifying EEG pathologies using ChronoNet)





## Results: Frequency Band importance (Identifying medications using DCNN)



## Conclusion and Future Work

- Spectral Perturbation is helpful to understand the importance of spectral bands
- The authors used training accuracies to make comparisons (flaw) which we changed in our methods
- The large size of the data is effective in building a robust model, However the model will not generalize or train effectively to a smaller dataset. We are interested in building models that can work in different data sizes.
- Used LSTM, DCNN, ChronoNet, LSTM autoencoder
- **Possible Solution:** Exploring denoising signal processing methods or Deep Learning methods like denoising Autoencoder to remove intrinsic and extrinsic artifacts

# Questions