

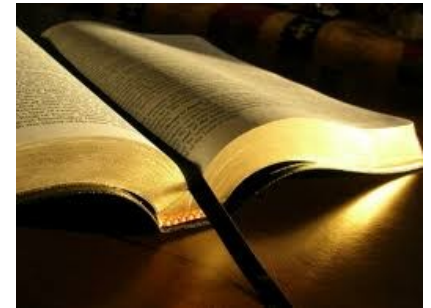
Summary:

Processing of kinematic data obtained from the Laboratory of Biomechanics of Lisbon in Matlab.

Kinematic analysis of a gait cycle in Matlab.

Suggested bibliography:

P. Nikravesh, *Computer-Aided Analysis of Mechanical Systems*, Prentice-Hall, Englewood-Cliffs, New Jersey, 1988.



1st Assignment: **Kinematic Analysis of a Biomechanical Model**

In this work, the Group is asked to study a gait cycle of one of its members (data collected in the Biomechanics Laboratory). The motion should be analyzed from the kinematics point of view and should be described using the directional terms and joint movement terminology presented in this course.

For the computational kinematic analysis of the human motion, the Group should:

- Define, using Cartesian coordinates, a 2D multibody model suitable for the motion under analysis.
- Identify the vector of generalized coordinates for the proposed model.
- Define the data driver constraints needed for the motion under analysis.
- Carry on the complete kinematic analysis of the model for the acquired motion.

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Kinematic Analysis of Multibody Systems

Laboratory data:

EMG data

The root-mean-square (RMS) envelopes of the EMG signals are provided along the raw data.

Kinematic and kinetic data

The coordinates of the bony landmarks and the ground reaction forces measured at the laboratory are provided.

Note: The ground reaction forces are provided in the local reference frame of each force plate (f_1 , f_2 , and f_3). The `tsv2mat.m` script must be used to transform the data to the same reference frame of the coordinates of the bony landmarks.

Foot pressure data

The distribution of foot pressures along the gait cycle are provided.

Gait parameters

The parameters most frequently used to characterize gait are provided.

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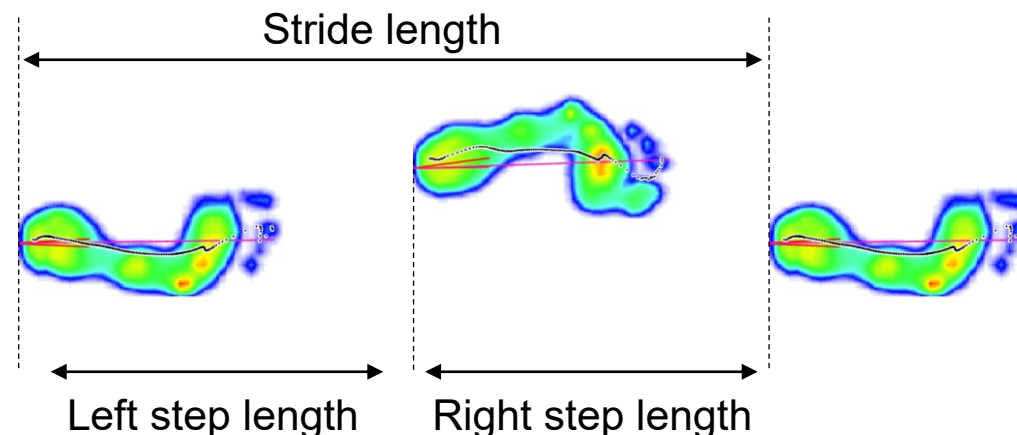
Kinematic Analysis of Multibody Systems

Laboratory data (gait parameters examples):

Step length is the distance between the heel contact point of one foot and that of the other foot.

Stride length is the distance between the successive heel contact points of one foot.

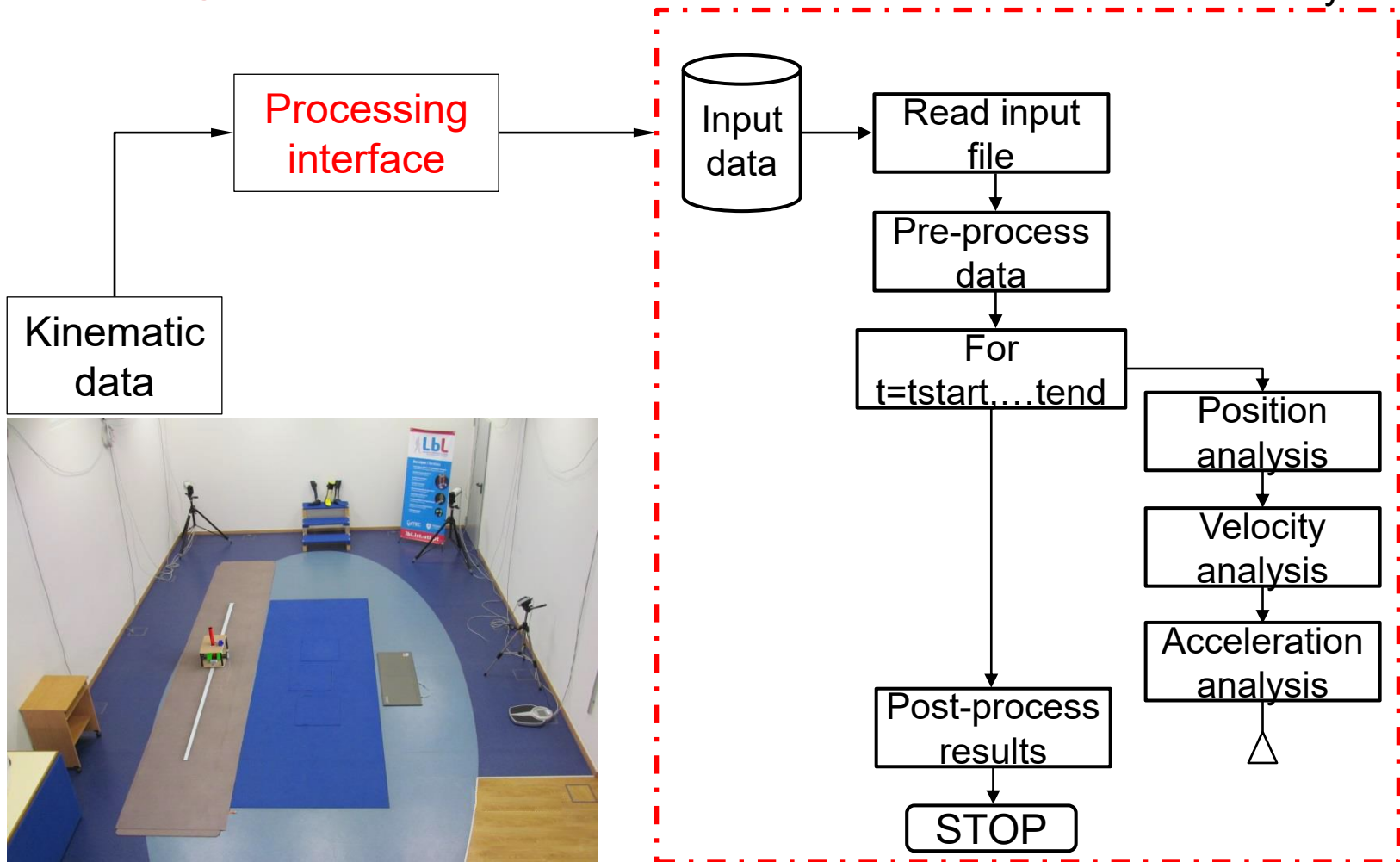
Cadence is the walking rate expressed in steps per minute. The average cadence is 100 – 115 steps/min.



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Kinematic Analysis of Multibody Systems

Laboratory data application:

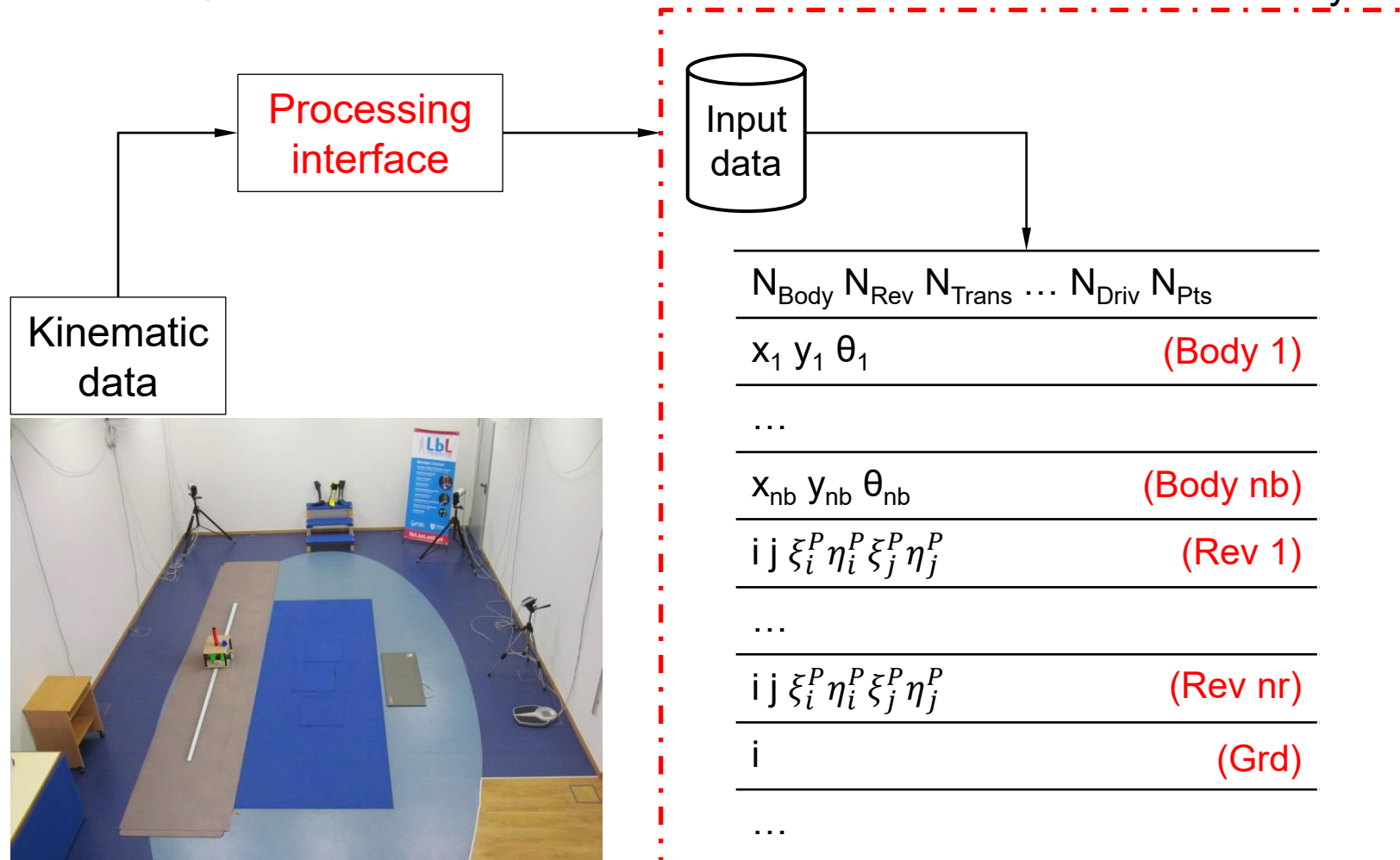


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Kinematic Analysis of Multibody Systems

Laboratory data application:

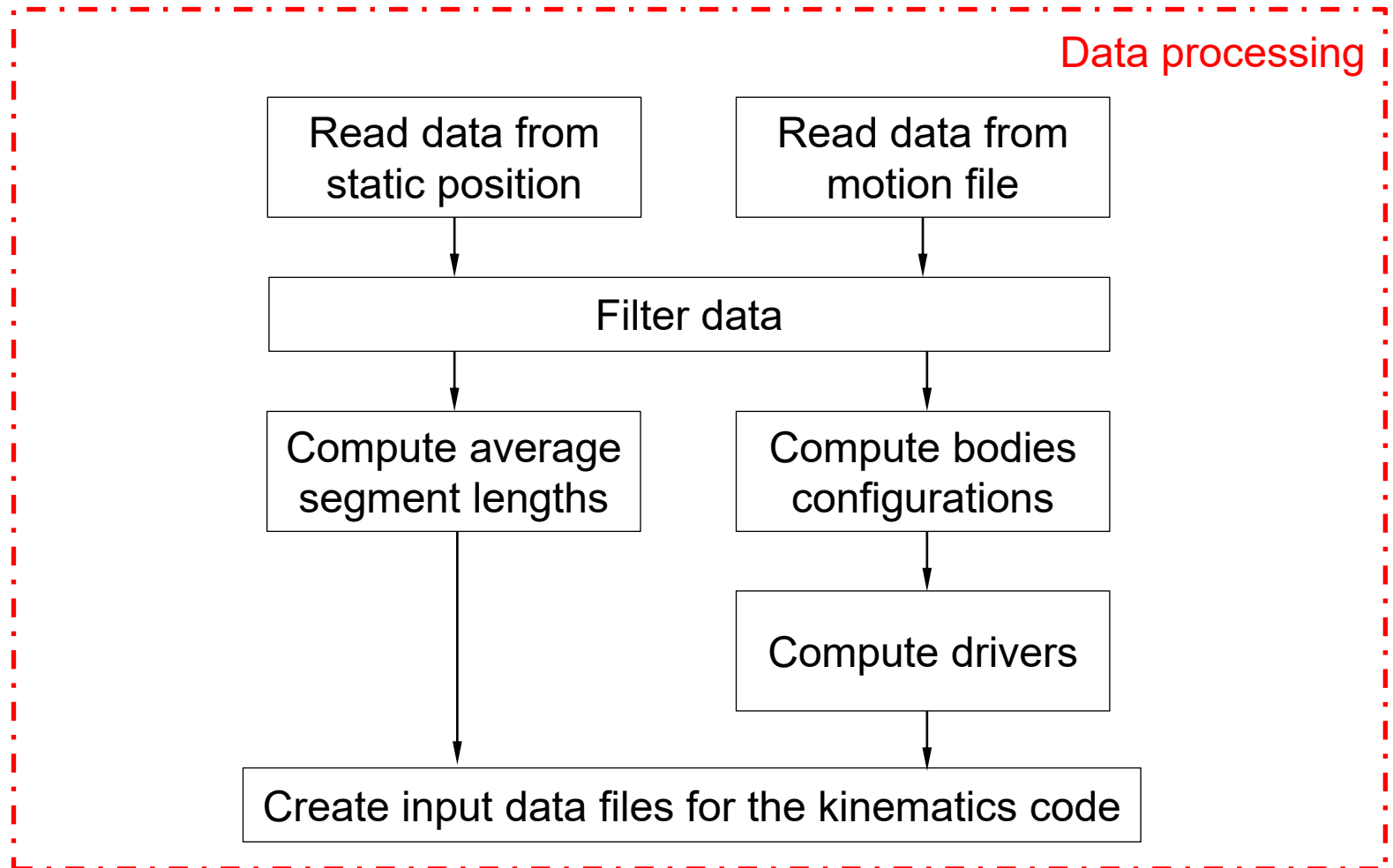
Kinematic analysis



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Kinematic Analysis of Multibody Systems

Flowchart of the data processing for the kinematic analysis:



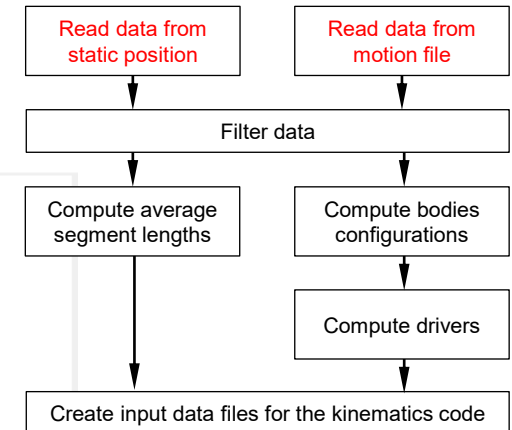
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Kinematic Analysis of Multibody Systems

Data structure:

```

NO_OF_FRAMES      932
NO_OF_CAMERAS     14
NO_OF_MARKERS     19
FREQUENCY         100
NO_OF_ANALOG      0
ANALOG_FREQUENCY  0
DESCRIPTION       --
TIME_STAMP        2017-11-03, 15:39:01      715118.94207204
DATA_INCLUDED     3D
MARKER_NAMES      1 - Head      2 - L_Shoulder  3 - L_Elbow    4 - L
685      6.84000  242.104  254.702  1701.632      208.881  400.142  1406.
686      6.85000  242.124  254.436  1701.640      209.215  400.072  1406.
687      6.86000  242.063  254.154  1701.725      209.506  400.038  1406.
688      6.87000  241.986  253.880  1701.731      209.870  400.035  1406.
689      6.88000  241.959  253.688  1701.777      210.284  400.053  1406.
690      6.89000  241.787  253.456  1701.674      210.760  400.012  1406.
691      6.90000  241.677  253.208  1701.681      211.224  400.016  1406.
692      6.91000  241.533  252.930  1701.591      211.635  400.061  1406.
693      6.92000  241.470  252.767  1701.568      212.103  399.978  1406.
694      6.93000  241.404  252.586  1701.514      212.474  399.958  1406.
695      6.94000  241.321  252.375  1701.492      212.766  399.790  1406.
  
```



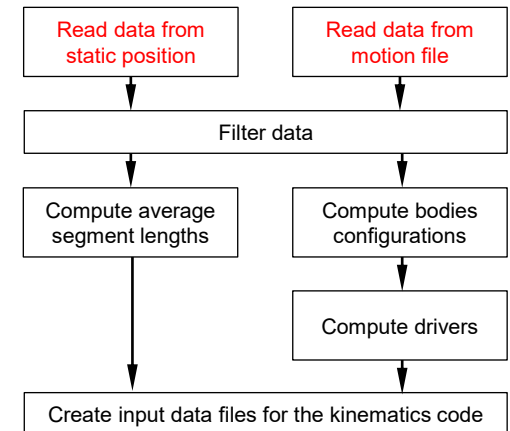
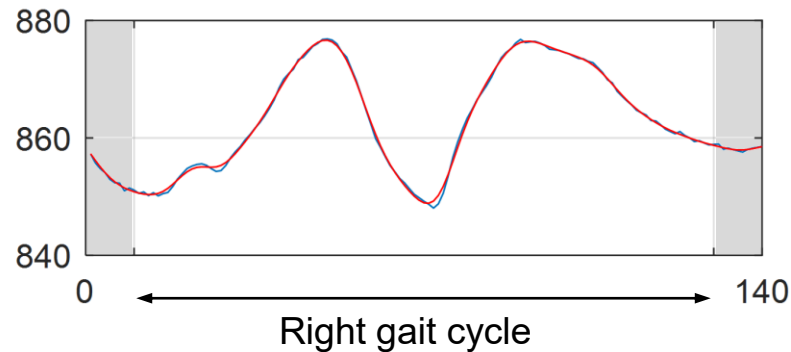
Notice that the coordinates are in the 3D space. For the application in the 2D space, the coordinates must be projected onto the sagittal plane.

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Kinematic Analysis of Multibody Systems

Data structure:

Note: The kinematic data provided for gait include 10 time steps before the beginning of the gait cycle and 10 time steps after.

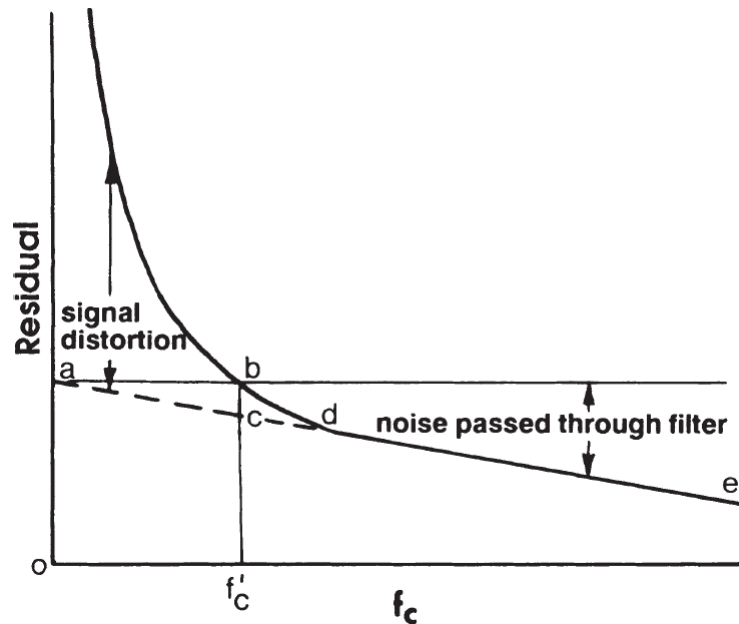


These time steps are included to have data for the filtering and spline interpolation steps before and after the gait cycle.

Data filtering:

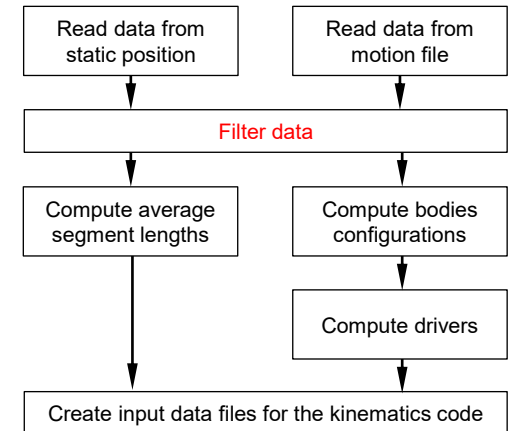
Low-pass filters are widely used to reduce noise levels in reconstructed trajectories.

Several methods exist to define the cut-off frequency (e.g., harmonic analysis, residual analysis).



$$R(f_c) = \sqrt{\frac{1}{N} \sum_{i=1}^N (X_i - \hat{X}_i)^2}$$

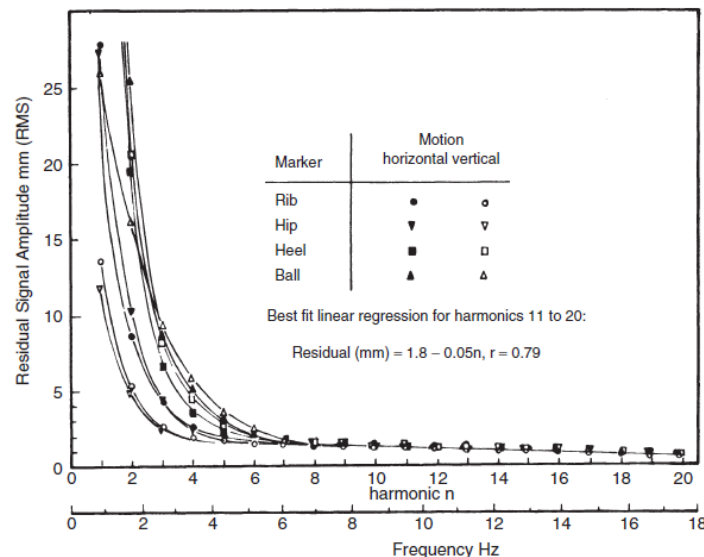
Plot of the residual between a filtered and an unfiltered signal as a function of the filter cutoff frequency; in Winter, 2009, Biomechanics and motor control of human movement.



Data filtering:

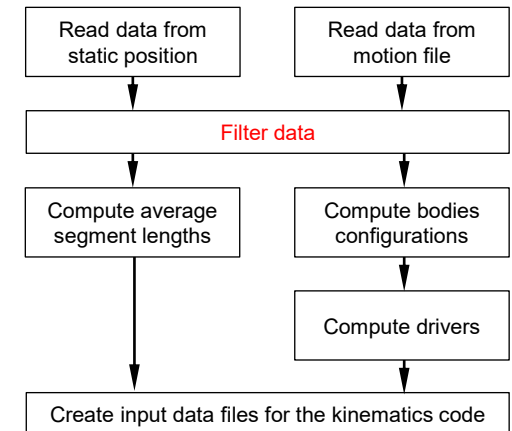
Low-pass filters are widely used to reduce noise levels in reconstructed trajectories.

Several methods exist to define the cut-off frequency (e.g., harmonic analysis, residual analysis).



$$R(f_c) = \sqrt{\frac{1}{N} \sum_{i=1}^N (X_i - \hat{X}_i)^2}$$

Plot of the residual of four markers from a walking trial; in Winter, 2009, Biomechanics and motor control of human movement.



The cut-off frequencies for a gait cycle are expected to range between 2 and 6 Hz.

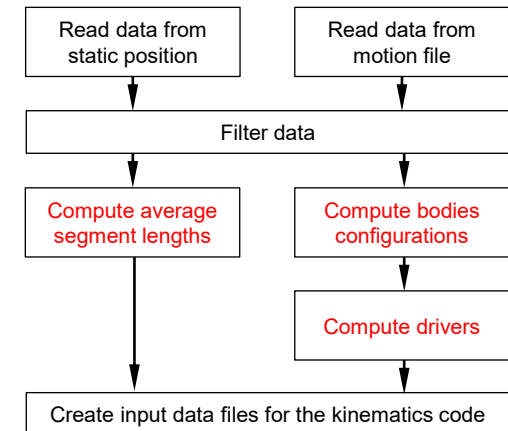
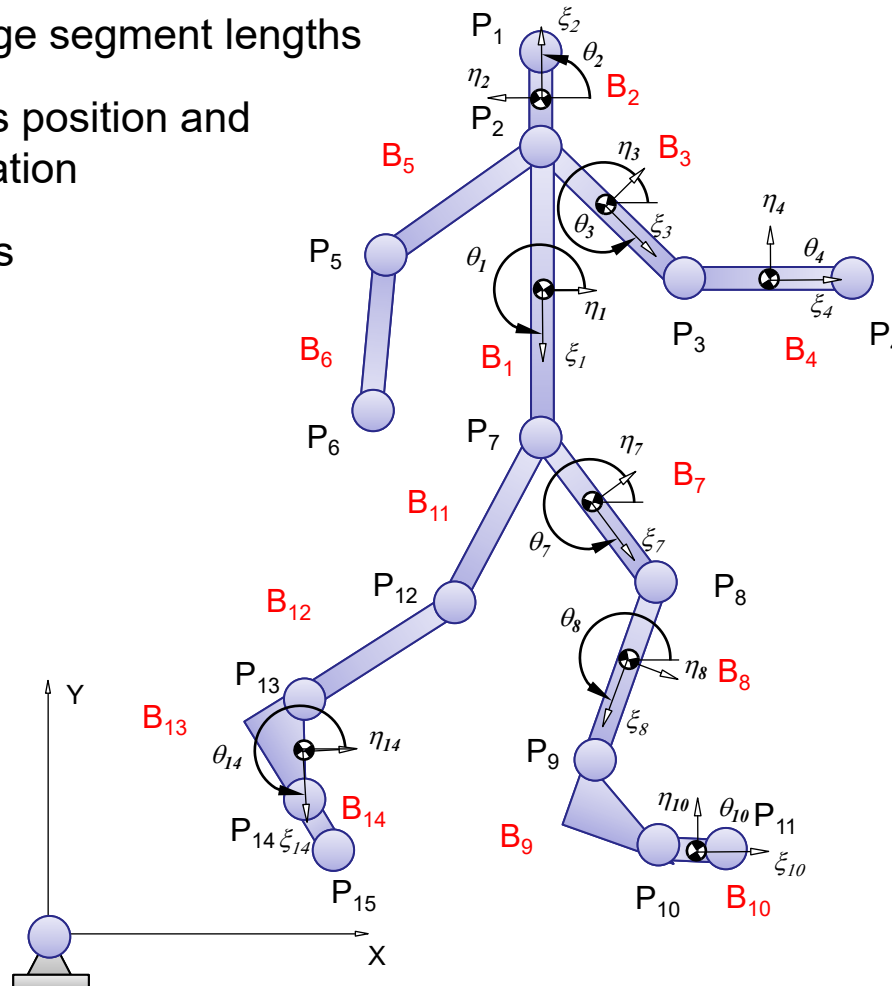
Kinematic Analysis of Multibody Systems

Compute biomechanical data:

Average segment lengths

Bodies position and orientation

Drivers



Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems

Segment lengths:

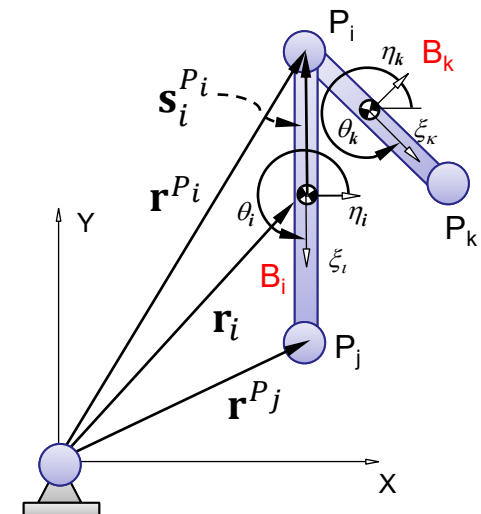
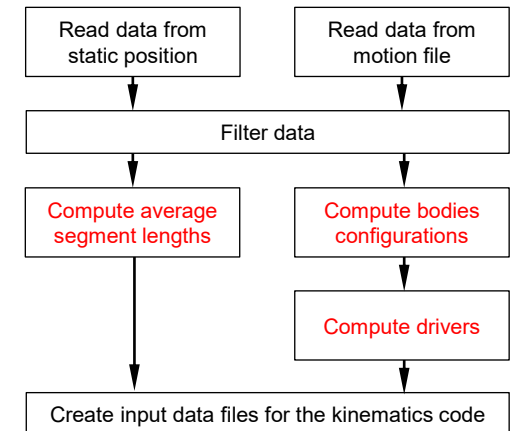
The length of body i is given by:

$$L_i = \sqrt{(\mathbf{r}^{P_j} - \mathbf{r}^{P_i})^T (\mathbf{r}^{P_j} - \mathbf{r}^{P_i})}$$

Due to measuring errors, the length of a segment will be different in each time frame. Therefore, an average length must be computed for each body:

$$L_i = \frac{\sum_{t=0}^{t_f} L_i^t}{n_f}$$

where n_f is the total number of frames.



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Kinematic Analysis of Multibody Systems

Position and orientation of the bodies:

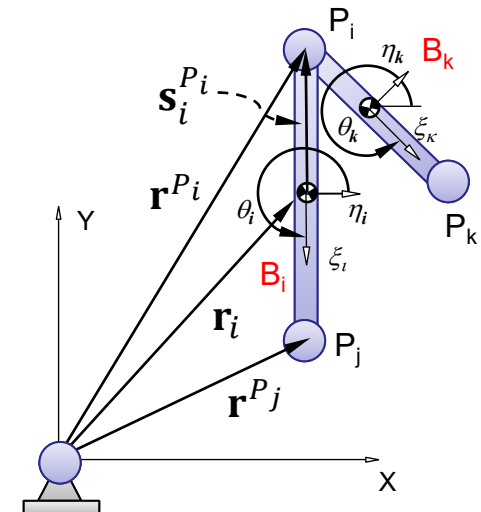
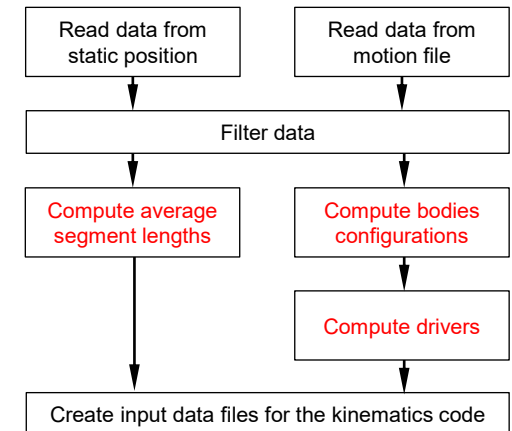
When using Cartesian coordinates, the coordinates required to define the position and orientation of a body are the position and orientation of a body-fixed reference frame:

$$\mathbf{q}_i = \begin{Bmatrix} \mathbf{r}_i \\ \theta_i \end{Bmatrix} = \begin{Bmatrix} x_i \\ y_i \\ \theta_i \end{Bmatrix}$$

The orientation of body i can be defined from points P_i and P_j :

$$\xi \text{ axis: } \frac{(\mathbf{r}^{P_j} - \mathbf{r}^{P_i})}{\sqrt{(\mathbf{r}^{P_j} - \mathbf{r}^{P_i})^T (\mathbf{r}^{P_j} - \mathbf{r}^{P_i})}}$$

$$\eta \text{ axis: } \perp \xi \text{ axis}$$



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Kinematic Analysis of Multibody Systems

Position and orientation of the bodies:

When using Cartesian coordinates, the coordinates required to define the position and orientation of a body are the position and orientation of a body-fixed reference frame:

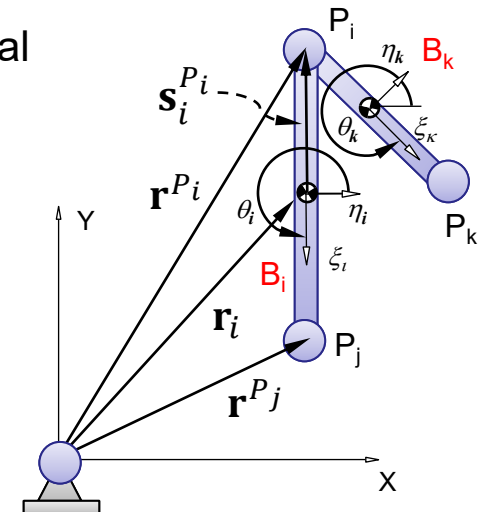
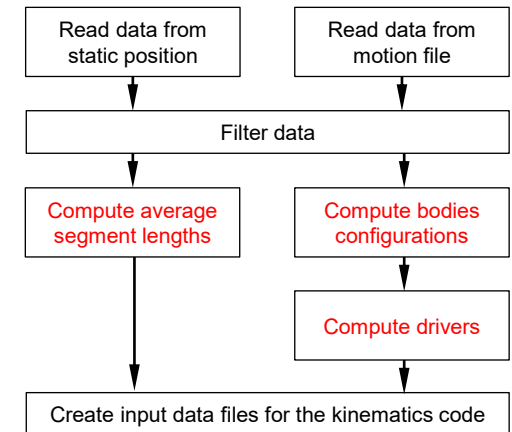
$$\mathbf{q}_i = \begin{Bmatrix} \mathbf{r}_i \\ \theta_i \end{Bmatrix} = \begin{Bmatrix} x_i \\ y_i \\ \theta_i \end{Bmatrix}$$

The position of the center of mass (CoM) can be defined using the relationships between the CoM and the proximal or distal points of the body:

$$\mathbf{r}^{P_i} = \mathbf{r}_i + \mathbf{A}_i \mathbf{s}_i^{P_i}$$

$$\Rightarrow \mathbf{r}_i = \mathbf{r}^{P_i} - \mathbf{A}_i \mathbf{s}_i^{P_i}$$

Note: Use an anthropometric table to define the relationships between CoM and the proximal or distal points of a body.



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Kinematic Analysis of Multibody Systems

Drivers:

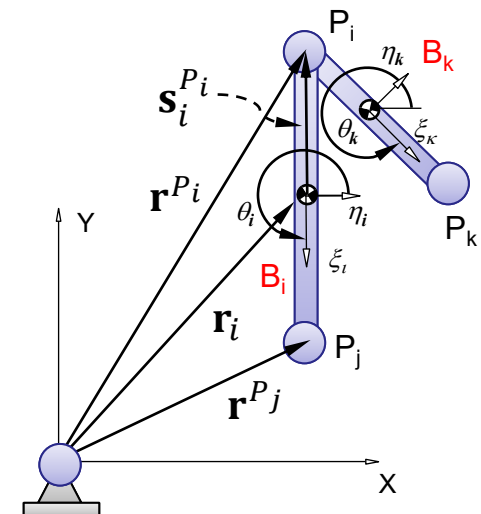
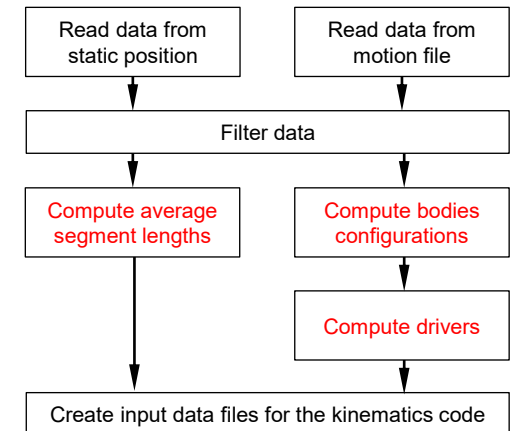
All degrees of freedom (dof) of the biomechanical model must be driven using the data measured in the laboratory.

Drivers' data should be computed considering the driver joints implemented in MuboKAP and MuboDAP.

The following drivers are particularly relevant:

$$\Phi^{(driv_{3,1})} = z - z^*(t),$$

$$\Phi^{(driv_{4,1})} = \theta_j - \theta_i - \theta_{ij}^*(t)$$



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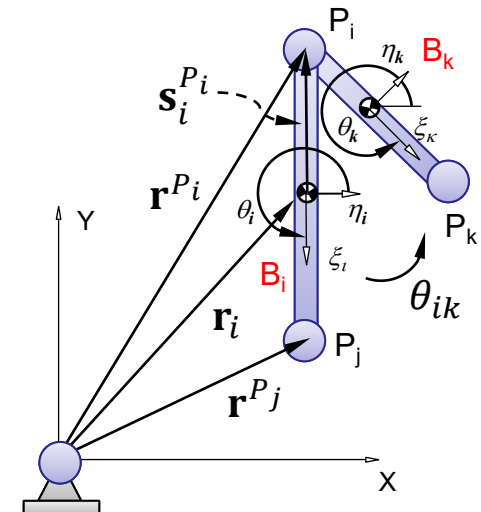
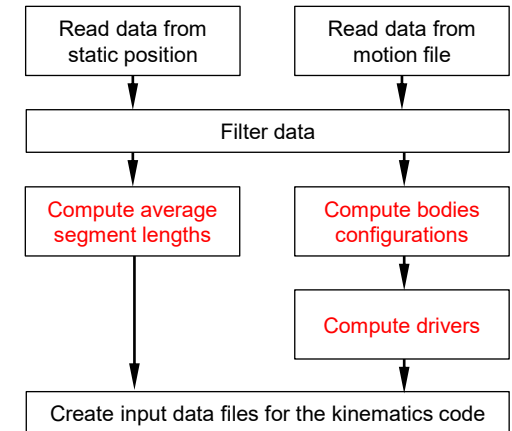
Kinematic Analysis of Multibody Systems

Drivers:

All degrees of freedom (dof) of the biomechanical model must be driven using the data measured in the laboratory.

Drivers' data should be written in *.txt files for the kinematics code to read. For instance, for the relative angle between bodies i and k :

t (s)	θ_{ik}^t (rad)
0	θ_{ik}^0
...	...
t_f	$\theta_{ik}^{t_f}$



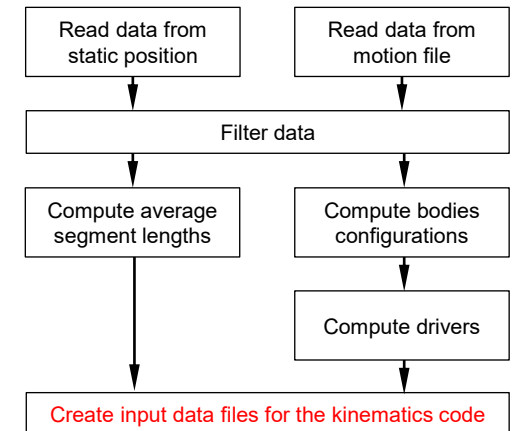
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Kinematic Analysis of Multibody Systems

Create input data files:

The input file of the biomechanical system to be read by the kinematic analysis and the drivers must be written:

N_{Body}	N_{Rev}	N_{Trans}	...	N_{Driv}	N_{Pts}	
x_1	y_1	θ_1				(Body 1)
...						
x_{nb}	y_{nb}	θ_{nb}				(Body nb)
i	j	ξ_i^P	η_i^P	ξ_j^P	η_j^P	(Rev 1)
...						
i	j	ξ_i^P	η_i^P	ξ_j^P	η_j^P	(Rev nr)
i						(Grd)
...						



t (s)	θ_{ik}^t (rad)
0	θ_{ik}^0
...	...
t_f	$\theta_{ik}^{t_f}$

Implementation tips (1):

Define the bodies and joints of the biomechanical model.

Identify the markers that define each body and its local reference frame:

P1 – Head

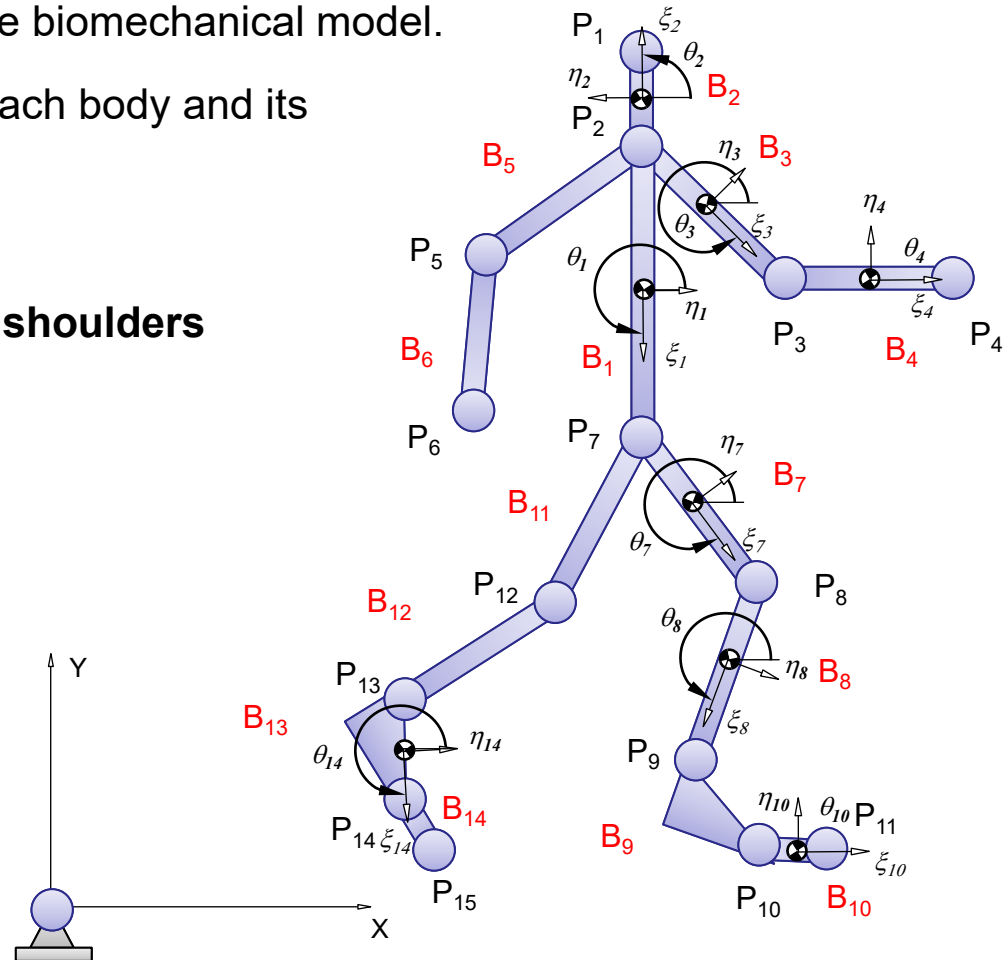
P2 – **Midpoint between shoulders**

P3 – Right elbow

P4 – Right wrist

P5 – Left elbow

...



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Kinematic Analysis of Multibody Systems

Implementation tips (2):

Considering a similar structure as that of the input file of the kinematics code, build a processing file to organize the data for the processing code.

Compute average segment lengths

Compute the position and orientation of the bodies for all time frames

Compute drivers

Processing file

N_{Body}	N_{Rev}	N_{Trans}	\dots	N_{Driv}	N_{Pts}
-------------------	------------------	--------------------	---------	-------------------	------------------

x_1	y_1	θ_1
-------	-------	------------

...

x_{nb}	y_{nb}	θ_{nb}
-----------------	-----------------	----------------------

i	j	ξ_i^P	η_i^P	ξ_j^P	η_j^P
-----	-----	-----------	------------	-----------	------------

...

i	j	ξ_i^P	η_i^P	ξ_j^P	η_j^P
-----	-----	-----------	------------	-----------	------------

i

...

Input file (kinematics code)

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Kinematic Analysis of Multibody Systems

Implementation tips (2):

Considering a similar structure as that of the input file of the kinematics code, build a processing file to organize the data for the processing code.

N_{Body}	N_{Rev}	N_{Trans}	\dots	N_{Driv}	N_{Pts}
P_2	P_7	ξ_1^{CoM}	$/L_1$		
\dots					
P_{m-1}	P_m	ξ_{nb}^{CoM}	$/L_{nb}$		
i	j	ξ_i^P	$/L_i$	η_i^P	$/L_i$
\dots					
k	l	ξ_k^P	$/L_k$	η_k^P	$/L_k$
i					
\dots					

Processing file

N_{Body}	N_{Rev}	N_{Trans}	\dots	N_{Driv}	N_{Pts}
x_1	y_1	θ_1			
\dots					
x_{nb}	y_{nb}	θ_{nb}			
i	j	ξ_i^P	η_i^P	ξ_j^P	η_j^P
\dots					
i	j	ξ_i^P	η_i^P	ξ_j^P	η_j^P
i					
\dots					

Input file (kinematics code)

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Kinematic Analysis of Multibody Systems

Anthropometry:

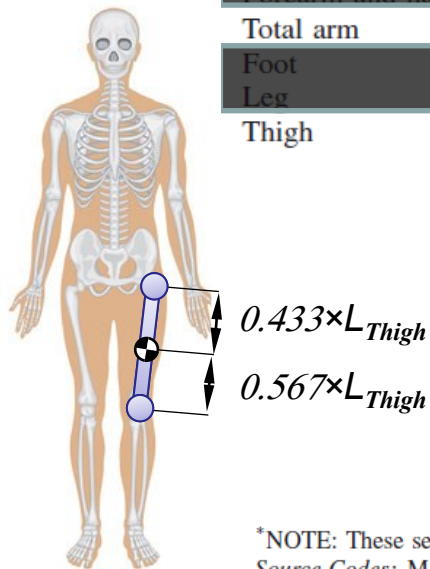
Segment	Definition	Segment Weight/Total Body Weight	Center of Mass/ Segment Length		Radius of Gyration/ Segment Length		
			Proximal	Distal	C of G	Proximal	Distal
Hand	Wrist axis/knuckle II middle finger	0.006 M	0.506	0.494 P	0.297	0.587	0.577 M
Forearm	Elbow axis/ulnar styloid	0.016 M	0.430	0.570 P	0.303	0.526	0.647 M
Upper arm	Glenohumeral axis/elbow axis	0.028 M	0.436	0.564 P	0.322	0.542	0.645 M
Forearm and hand	Elbow axis/ulnar styloid	0.022 M	0.682	0.318 P	0.468	0.827	0.565 P
Total arm	Glenohumeral joint/ulnar styloid	0.050 M	0.530	0.470 P	0.368	0.645	0.596 P
Foot	Lateral malleolus/head metatarsal II	0.0145 M	0.50	0.50 P	0.475	0.690	0.690 P
Leg	Femoral condyles/medial malleolus	0.0465 M	0.433	0.567 P	0.302	0.528	0.643 M
Thigh	Greater trochanter/femoral condyles	0.100 M	0.433	0.567 P	0.323	0.540	0.653 M
Foot and leg	Femoral condyles/medial malleolus	0.061 M	0.606	0.394 P	0.416	0.735	0.572 P
Total leg	Greater trochanter/medial malleolus	0.161 M	0.447	0.553 P	0.326	0.560	0.650 P
Head and neck	C7–T1 and 1st rib/ear canal	0.081 M	1.000	— PC	0.495	0.116	— PC
Shoulder mass	Sternoclavicular joint/glenohumeral axis	—	0.712	0.288	—	—	—
Thorax	C7–T1/T12–L1 and diaphragm*	0.216 PC	0.82	0.18	—	—	—
Abdomen	T12–L1/L4–L5*	0.139 LC	0.44	0.56	—	—	—
Pelvis	L4–L5/greater trochanter*	0.142 LC	0.105	0.895	—	—	—
Thorax and abdomen	C7–T1/L4–L5*	0.355 LC	0.63	0.37	—	—	—
Abdomen and pelvis	T12–L1/greater trochanter*	0.281 PC	0.27	0.73	—	—	—
Trunk	Greater trochanter/glenohumeral joint*	0.497 M	0.50	0.50	—	—	—
Trunk head neck	Greater trochanter/glenohumeral joint*	0.578 MC	0.66	0.34 P	0.503	0.830	0.607 M
Head, arms, and trunk (HAT)	Greater trochanter/glenohumeral joint*	0.678 MC	0.626	0.374 PC	0.496	0.798	0.621 PC
HAT	Greater trochanter/mid rib	0.678	1.142	—	0.903	1.456	—

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Kinematic Analysis of Multibody Systems

Anthropometry:

Segment	Definition	Segment Weight/Total Body Weight	Center of Mass/ Segment Length		Radius of Gyration/ Segment Length		
			Proximal	Distal	C of G	Proximal	Distal
Hand	Wrist axis/knuckle II middle finger	0.006 M	0.506	0.494 P	0.297	0.587	0.577 M
Forearm	Elbow axis/ulnar styloid	0.016 M	0.430	0.570 P	0.303	0.526	0.647 M
Upper arm	Glenohumeral axis/elbow axis	0.028 M	0.436	0.564 P	0.322	0.542	0.645 M
Forearm and hand	Elbow axis/ulnar styloid	0.022 M	0.682	0.318 P	0.468	0.827	0.565 P
Total arm	Glenohumeral joint/ulnar styloid	0.050 M	0.530	0.470 P	0.368	0.645	0.596 P
Foot	Lateral malleolus/head metatarsal II	0.0145 M	0.50	0.50 P	0.475	0.690	0.690 P
Leg	Femoral condyles/medial malleolus	0.0465 M	0.433	0.567 P	0.302	0.528	0.643 M
Thigh	Greater trochanter/femoral condyles	0.100 M	0.433	0.567 P	0.323	0.540	0.653 M



*NOTE: These segments are presented relative to the length between the greater trochanter and the glenohumeral joint.

Source Codes: M, Dempster via Miller and Nelson; *Biomechanics of Sport*, Lea and Febiger, Philadelphia, 1973. P, Dempster via Plagenhoef; *Patterns of Human Motion*, Prentice-Hall, Inc. Englewood Cliffs, NJ, 1971. L, Dempster via Plagenhoef from living subjects; *Patterns of Human Motion*, Prentice-Hall, Inc., Englewood Cliffs, NJ, 1971. C, Calculated.

Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems

Matlab code – main function:

```
|clear all
% Pre-processing of data from the Laboratory of Biomechanics of Lisbon

% Reads input data for the biomechanical model
ReadInput('ProcessingFile.txt');

% Reads the static data
StaticData = ReadProcessData('sta0001_static.tsv');

% Compute the average segment lengths
ComputeAverageLengths(StaticData);

% Reads the gait data
GaitData = ReadProcessData('sta0001_PD1.tsv');

% Computes the positions and angles of the body
EvaluatePositions(GaitData);

% Evaluates the drivers
EvaluateDrivers(GaitData);

% Updates the data in the files to be read by the kinematic analysis
WritesModelInput('BiomechanicalModel.txt');
```


Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems

Matlab code – ReadInput (excerpts):

```
function ReadInput(FileName)
```

```
% ...
```

```
global NBody Body Jnt Pts
```

```
% Read the input file
```

```
H = dlmread(FileName);
```

```
%... Initialize data
```

```
Nline = 1;
```

```
%% ... Store data in Local Variables
```

```
NBody = H(Nline, 1);
```

```
Jnt.NRevolute = H(Nline, 2);
```

```
Jnt.NTranslation = H(Nline, 3);
```

```
Jnt.NRevRev = H(Nline, 4);
```

```
Jnt.NTraRev = H(Nline, 5);
```

```
Jnt.NCam = H(Nline, 6);
```

```
Jnt.NGround = H(Nline, 7);
```

```
Jnt.NSimple = H(Nline, 8);
```

```
Jnt.NDriver = H(Nline, 9);
```

```
Pts.NPointsInt = H(Nline, 10);
```

```
%% ... Store initial positions for Rigid Bodies
```

```
for i = 1 : NBody
```

```
    Nline = Nline + 1;
```

```
    Body(i).pi = H(Nline, 1);
```

```
    Body(i).pj = H(Nline, 2);
```

```
    Body(i).PCoM = H(Nline, 3);
```

```
end
```

```
%... Store information for Revolute Joints
```

```
for k = 1 : Jnt.NRevolute
```

```
    Nline = Nline + 1;
```

```
    Jnt.Revolute(k).i = H(Nline, 1);
```

```
    Jnt.Revolute(k).j = H(Nline, 2);
```

```
    Jnt.Revolute(k).spi = H(Nline, 3:4)';
```

```
    Jnt.Revolute(k).spj = H(Nline, 5:6)';
```

```
end
```

```
%... Store information for Driver Constraints
```

```
for k = 1:Jnt.NDriver
```

```
    Nline = Nline + 1;
```

```
    Jnt.Driver(k).type = H(Nline,1);
```

```
    Jnt.Driver(k).i = H(Nline,2);
```

```
    Jnt.Driver(k).coortype = H(Nline,3);
```

```
    Jnt.Driver(k).j = H(Nline,4);
```

```
    if (Jnt.Driver(k).type ~= 3 &&...
```

```
        Jnt.Driver(k).type ~= 4 &&...
```

```
        Jnt.Driver(k).type ~= 5)
```

```
        disp('Type of driver not implemented');
```

```
    else
```

```
        Jnt.Driver(k).spPi = H(Nline,5:6)';
```

```
        Jnt.Driver(k).spPj = H(Nline,7:8)';
```

```
        Jnt.Driver(k).order = H(Nline,9); % order of spline
```

```
        Jnt.Driver(k).Filename = H(Nline,10);
```

```
    end
```

```
end
```

...

Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems

Matlab code – ReadProcessData (excerpts):

Filtering

```
% Cut off frequency
Wn = (2 * FinalCutOff) / SamplingFrequency;

% Butterworth parameters
[Ab, Bb] = butter(2, Wn, 'low');

% Filtering of the data with a zero phase lag filter
FilteredData = filtfilt(Ab, Bb, Data);
```

```
% Organizes the data according to the definition of the biomechanical model
% Notice that the coordinates from the lab are organized as follows:
% 1 - Head; % 2 - L_Shoulder; % 3 - L_Elbow; % 4 - L_Wrist; % 5 - R_Shoulder
% 6 - R_Elbow; % 7 - R_Wrist; % 8 - L_Hip; % 9 - L_Knee; % 10 - L_Ankle;
% 11 - L_Heel; % 12 - L_Meta_V; % 13 - L_Toe_II; % 14 - R_Hip; % 15 - R_Knee
% 16 - R_Ankle; % 17 - R_Heel; % 18 - R_Meta_V; % 19 - R_Toe_II
LabData.Coordinates = [FilteredCoordinates(:,1:2),... % Head
    (FilteredCoordinates(:,3:4) + FilteredCoordinates(:,9:10)) / 2,... % Midpoint between shoulders
    FilteredCoordinates(:,11:12),... % Right elbow
    FilteredCoordinates(:,13:14),... % Right wrist
    FilteredCoordinates(:,5:6),... % Left elbow
    FilteredCoordinates(:,7:8),... % Left wrist
    (FilteredCoordinates(:,15:16) + FilteredCoordinates(:,27:28)) / 2,... % Midpoint between hips
    FilteredCoordinates(:,29:30),... % Right knee
    FilteredCoordinates(:,31:32),... % Right ankle
    FilteredCoordinates(:,35:36),... % Right metatarsal
    FilteredCoordinates(:,37:38),... % Right hallux
    FilteredCoordinates(:,17:18),... % Left knee
    FilteredCoordinates(:,19:20),... % Right ankle
    FilteredCoordinates(:,23:24),... % Right metatarsal
    FilteredCoordinates(:,25:26)] * 1e-3; % Right hallux
```

P₁
P₂
P₃

...

Organization
of the data

Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems

Matlab code – ReadProcessData:

A double filtering procedure (double pass) is required to remove phase shift.



Zero-phase filtering versus conventional filtering; in Mathworks documentation, `filtfilt` function.

Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems

Matlab code – ComputeAverageLengths (excerpt):

```
% Number of frames to evaluate
NFrames = size(LabData.Coordinates, 1);

for i = 1 : NBody

    % Allocates memory for the lengths
    SegmentLength = zeros(NFrames, 1);

    % Goes through all frames
    for j = 1 : NFrames

        % Position of the coordinates of points Pi and Pj
        Pi = 2 * (Body(i).pi - 1) + 1;
        Pj = 2 * (Body(i).pj - 1) + 1;

        % Computes the length for the current frame
        SegmentLength(j) = norm(LabData.Coordinates(j, Pi : Pi + 1) - ...
                                LabData.Coordinates(j, Pj : Pj + 1));

        % End of the loop that goes through all frames
    end

    % Defines the average length
    Body(i).Length = mean(SegmentLength);

    % End of the loop that goes through all bodies
end
```

Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems (Review)

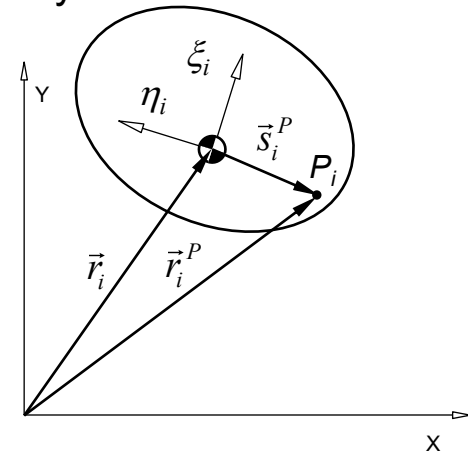
Modeling with Cartesian coordinates:

The position of a point belonging to a rigid body i is described by:

$$\mathbf{r}_i^P = \mathbf{r}_i + \mathbf{s}_i^P$$

It is convenient to express positions of points of a rigid body in coordinates of the body-fixed coordinate frame

$$\mathbf{s}_i^P = \mathbf{A}_i \mathbf{s}_i'^P \Rightarrow s_i^P = \begin{bmatrix} \cos\theta_i & -\sin\theta_i \\ \sin\theta_i & \cos\theta_i \end{bmatrix} \begin{Bmatrix} \xi_i \\ \eta_i \end{Bmatrix}$$



The following quantities are broadly used in the formulation of all methods addressed in this course:

$$\mathbf{r}_i^P = \{x_i^P \quad y_i^P\}^T$$

Global position of point P belonging to body i

$$\mathbf{A}_i = \begin{bmatrix} \cos\theta_i & -\sin\theta_i \\ \sin\theta_i & \cos\theta_i \end{bmatrix}$$

Transformation matrix of body i

$$\mathbf{s}_i'^P = \{\xi_i^P \quad \eta_i^P\}^T$$

Position of point P in the body-fixed frame of body i

Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems (Review)

Kinematic Analysis:

Position analysis (requires solving a system of nonlinear equations using, for instance, the Newton-Raphson Method):

$$\Phi(\mathbf{q}, t) = \mathbf{0} \Rightarrow \begin{cases} \mathbf{q}_{i+1} = \mathbf{q}_i - [\Phi_{\mathbf{q}_i}(\mathbf{q}_i, t)]^{-1} \Phi(\mathbf{q}_i, t) \\ |\mathbf{q}_i - \mathbf{q}_{i+1}| \leq \varepsilon \end{cases}$$

$$\Phi_{\mathbf{q}}(\mathbf{q}_i) = \begin{bmatrix} \frac{\partial \Phi_1}{\partial q_1} & \dots & \frac{\partial \Phi_1}{\partial q_n} \\ \vdots & \ddots & \vdots \\ \frac{\partial \Phi_n}{\partial q_1} & \dots & \frac{\partial \Phi_n}{\partial q_n} \end{bmatrix}$$

Velocity analysis (requires solving a system of linear equations):

$$\dot{\Phi}(\mathbf{q}, t) \equiv \Phi_{\mathbf{q}} \dot{\mathbf{q}} = \mathbf{v}$$

$$\mathbf{v} = - \frac{\partial \Phi}{\partial t}$$

Acceleration analysis (requires solving a system of linear equations):

$$\ddot{\Phi}(\mathbf{q}, \dot{\mathbf{q}}, t) \equiv \Phi_{\mathbf{q}} \ddot{\mathbf{q}} = \gamma$$

$$\gamma = - \frac{\partial^2 \Phi}{\partial t^2} - (\Phi_{\mathbf{q}} \dot{\mathbf{q}})_{\mathbf{q}} \dot{\mathbf{q}}$$

Week 03, Laboratory 03

Kinematic Analysis of Multibody Systems

Homework Exercise :

Considering the coordinates $\mathbf{r}_1 = \{x_1 \ y_1\}^T$, and θ_1 for the arm segment:

- If $\mathbf{r}_1 = \left\{\frac{\sqrt{2}}{4} \ \frac{\sqrt{2}}{4}\right\}^T$, $\theta_1 = \frac{\pi}{4}$, and $\mathbf{s}'^{P_2}_1 = \left\{\frac{1}{2} \ 0\right\}^T$, compute the global coordinates of point P_2 .
- If $\mathbf{r}^{P_3}_1 = \left\{\frac{\sqrt{2}}{16} \ 0\right\}^T$, determine the local coordinates of Point P_3 .
- Determine the number of dof of the system. Write the constraint equations. For the driver constraint, consider that the body is rotating with a frequency w ($\Phi^{driv} = \theta_1 - wt$).
- Determine the Jacobian matrix and write the velocity and acceleration equations for the system.

