



Introduction

- Background
 - Stroke is a leading cause of motor deficit
 - Every year, approximately **795,000** people experience a new or recurrent stroke in the US
 - Motor function can be recovered through physical rehabilitation
 - Traditional physical rehabilitation assessment has two major drawbacks
 - Assessment is based on the clinicians' subjective judgments
 - Standard clinical rating scales such as Fugl-Meyer Assessment (FMA) and Wolf Motor Function Test (WMFT) can not provide the details of motor performance
- Problem Statement
 - Develop a quantitative method to automatically analyze and evaluate post-stroke motor function
- Challenges
 - Need a tool to precisely capture patients' physical motion
 - Need to build a motion model that is able to capture the details of motor behavior

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Data Collection

- Participants
 - 2 patients with limb hemiparesis from stroke are recruited at **Precision Rehabilitation Center** at Long Beach and **Rancho Los Amigos National Rehabilitation Center** at Downey
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- Motor Tasks
 - 5 upper limb motor tasks from the Fugl-Meyer Assessment (FMA) are performed
 - Flex Synergy
 - Hand Behind Back
 - Shoulder Flexion to 90 degree
 - Shoulder Flexion from 90 to 180 degree
 - Pronation / Supination Elbow Flexed
 - Each participant performed each motor task 6 times
 - Each task was assigned a score based on the FMA scale (0, 1, 2) by a physical therapist

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Our Method

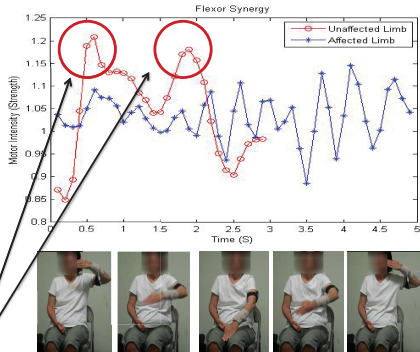
- Wearable Motion Sensor
 - 3-axis accelerometer ($\pm 6g$), 3-axis gyroscope ($\pm 500dps$)
 - Sampling rate: 100 Hz
- Fine-Grained Post-Stroke Motor Function Analysis Framework
 - Sliding Window
 - Feature Extraction
 - Pattern Recognition



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Results

- Motor Task:
 - Flexor Synergy
- Horizontal Axis:
 - Time (Second)
- Vertical Axis:
 - Motion Intensity
- Unaffected limb:
 - Red curve
 - FMA score: 12/12
- Affected limb:
 - Blue curve
 - FMA score: 8/12
- There exist two peaks for the unaffected limb which do not appear for the affected limb



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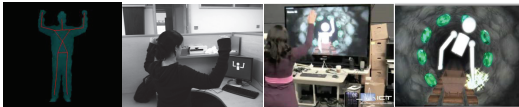
Details

- Small Window Cell
 - Divide the streaming sensor data from each motor task segment into a sequence of fixed length window cells whose length is much smaller than the duration of the motor task (0.1 second)
- Feature Extraction
 - Extracted from each window cell to form a local feature vector
 - Features that capture the intrinsic characteristics of the motor behavior. Examples include:
 - Motion Intensity (MI): $MI(t) = \sqrt{a_x(t)^2 + a_y(t)^2 + a_z(t)^2}$
 - Normalized Signal Magnitude Area (SMA): $SMA = \frac{1}{T} \left(\sum_{t=1}^T |a_x(t)| + \sum_{t=1}^T |a_y(t)| + \sum_{t=1}^T |a_z(t)| \right)$
 - Averaged Rotation Energy (ARE): The mean value of the energy over three gyroscope axes
 - Each motor task segment is then transformed into a sequence of local feature vectors, which forms a trajectory in the feature space
- Pattern Recognition
 - Extract pattern interesting to physical therapists

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Conclusion and Future Work

- Conclusion
 - We present a methodology for fine-grained assessments of post-stroke motion functionalities using wearable motion sensors
 - Our approach provides quantitative evaluations on motor function based on sensor signals and acts as a significant complement to the standard clinical rating scales
- Future Work
 - Build a large dataset to include more patients
 - Develop signal processing algorithms to automatically capture patterns that are important to physical therapists to track patients' progress during rehabilitation
 - Integrate with other sensing modalities, such as vision sensor (Microsoft Kinect)



Images from Kinect-based rehabilitation tool: Jewel Mine, developed at USC Institute for Creative Technologies

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