

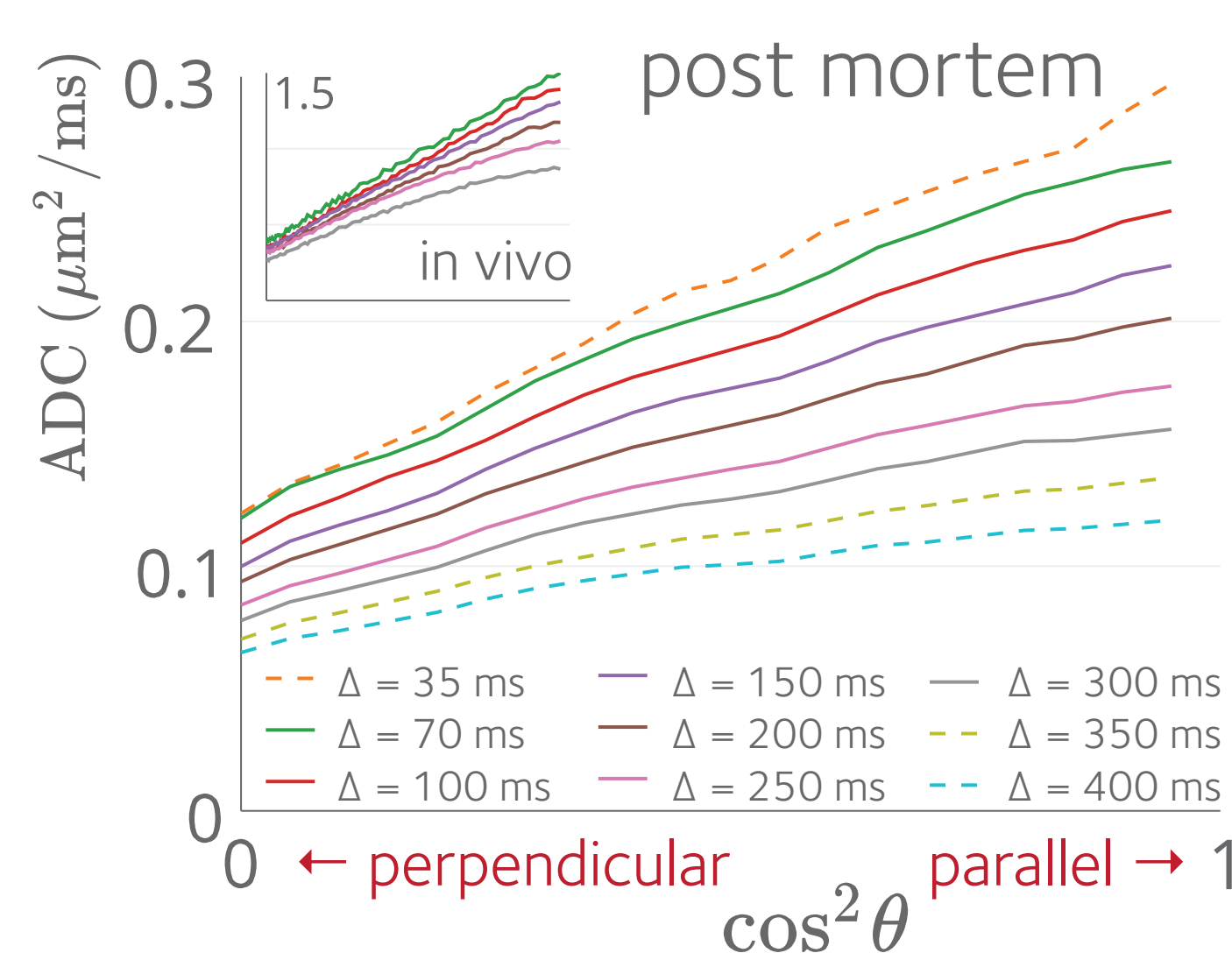
BACKGROUND

- Diffusion imaging at long diffusion times (Δ) informs on micro-structural tissue features up to the $\sim 100 \mu\text{m}$ scale.
- Approximation of axons as straight cylinders might not hold, even for tissues that are generally assumed to be coherently organized, for example: the human corpus callosum (CC).
- Electron microscopy (Mikula 2012) and histology (Budde 2013) suggest that the CC is far from coherent: fibres bend, twist and undulate which might lead to specific signatures of hindrance along the tract.
- In this study, we investigated the diffusion time dependence of the apparent diffusion coefficient (ADC) along the fibres in the CC.
- Biophysical mechanisms of this dependence are explored by Monte Carlo simulations of various tissue models.

DIFFUSION TIME DEPENDENCE OF THE ADC IN THE CORPUS CALLOSUM

- The ADC in the corpus callosum decreases with diffusion time; to a comparable degree across and along the tract.
- This suggests considerable diffusion hindrance not only perpendicular to the fibres, but also in the tract direction.
- A model of infinitely long straight cylinders might thus be inappropriately simple, even for the (supposedly) most coherent WM tract.

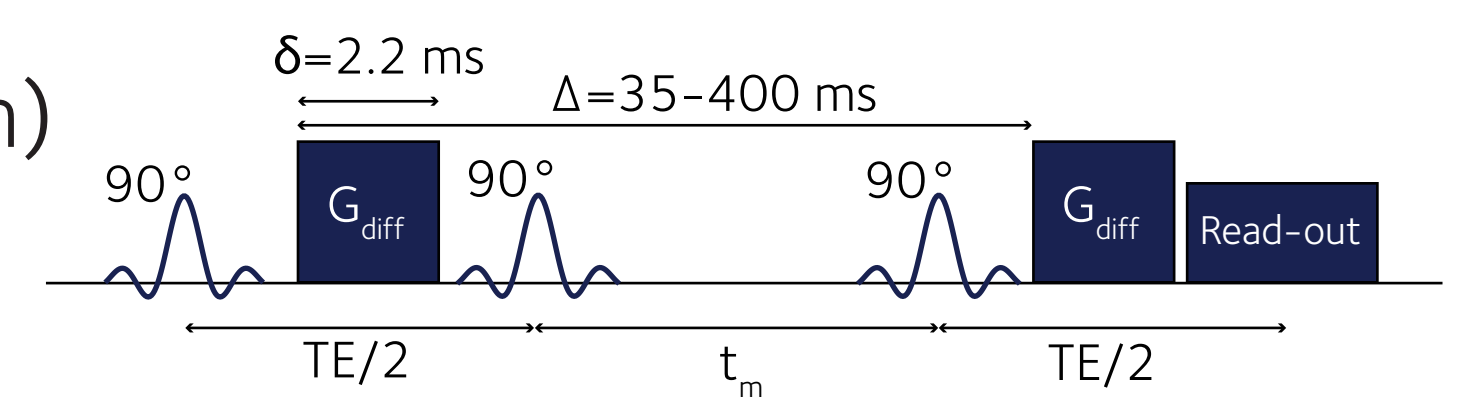
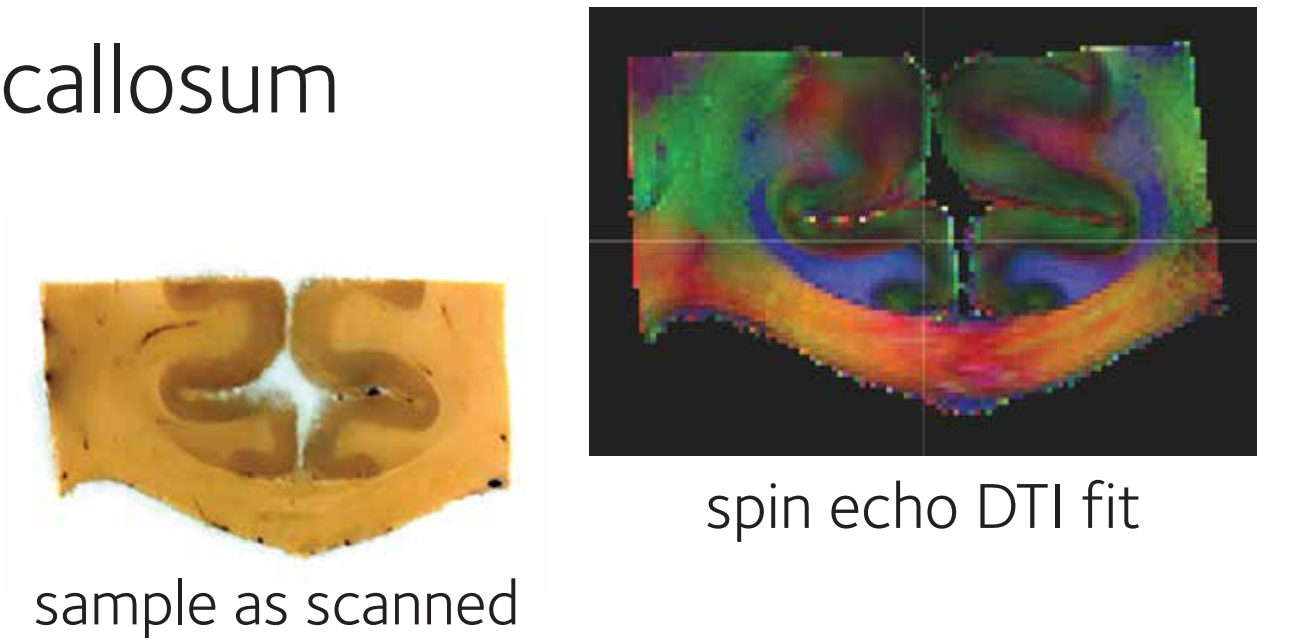
Figure 1. ADC plotted against \cos^2 of the angle between the diffusion gradient direction and the primary diffusion direction.





METHODS

MR MEASUREMENTS (POST MORTEM)

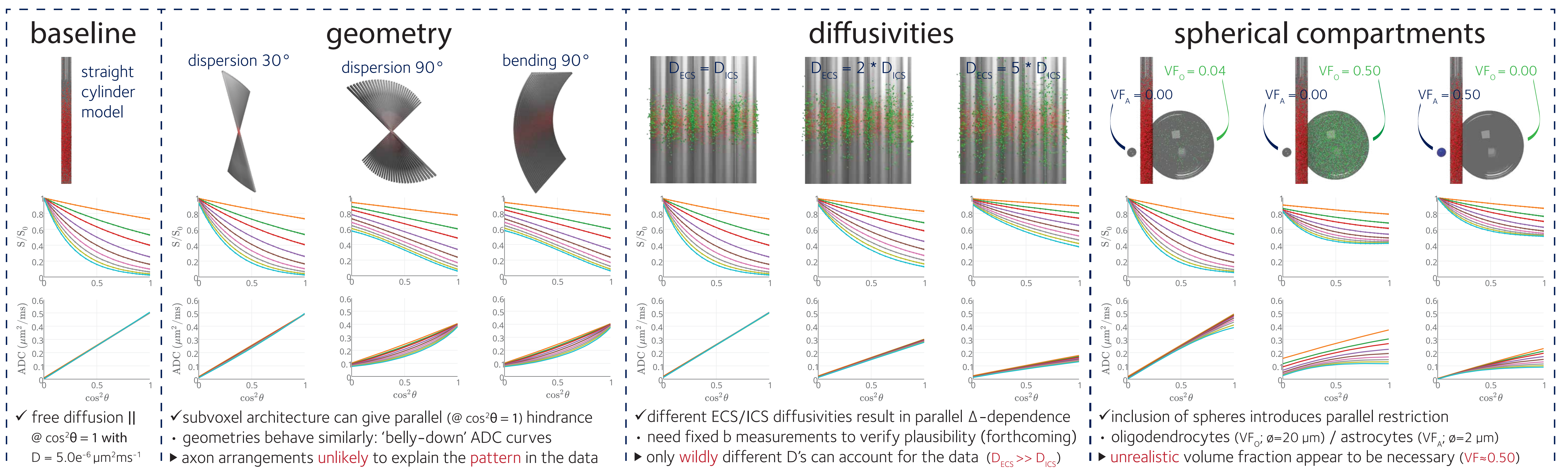
- 3x2 cm coronal block of a human corpus callosum
- soaked in PBS for 72h
- scanned in Fluorinert on a Varian 9.4T
- acquiring DW-STEAM data with:
 - 9 diffusion times: 35-400 ms
 - 30 directions
 - fixed q-value ($0.14 \text{ rad}/\mu\text{m}$)
 - TE=16 ms, TR=2.4-4.1 s
 - 10 slices, 400 μm voxels



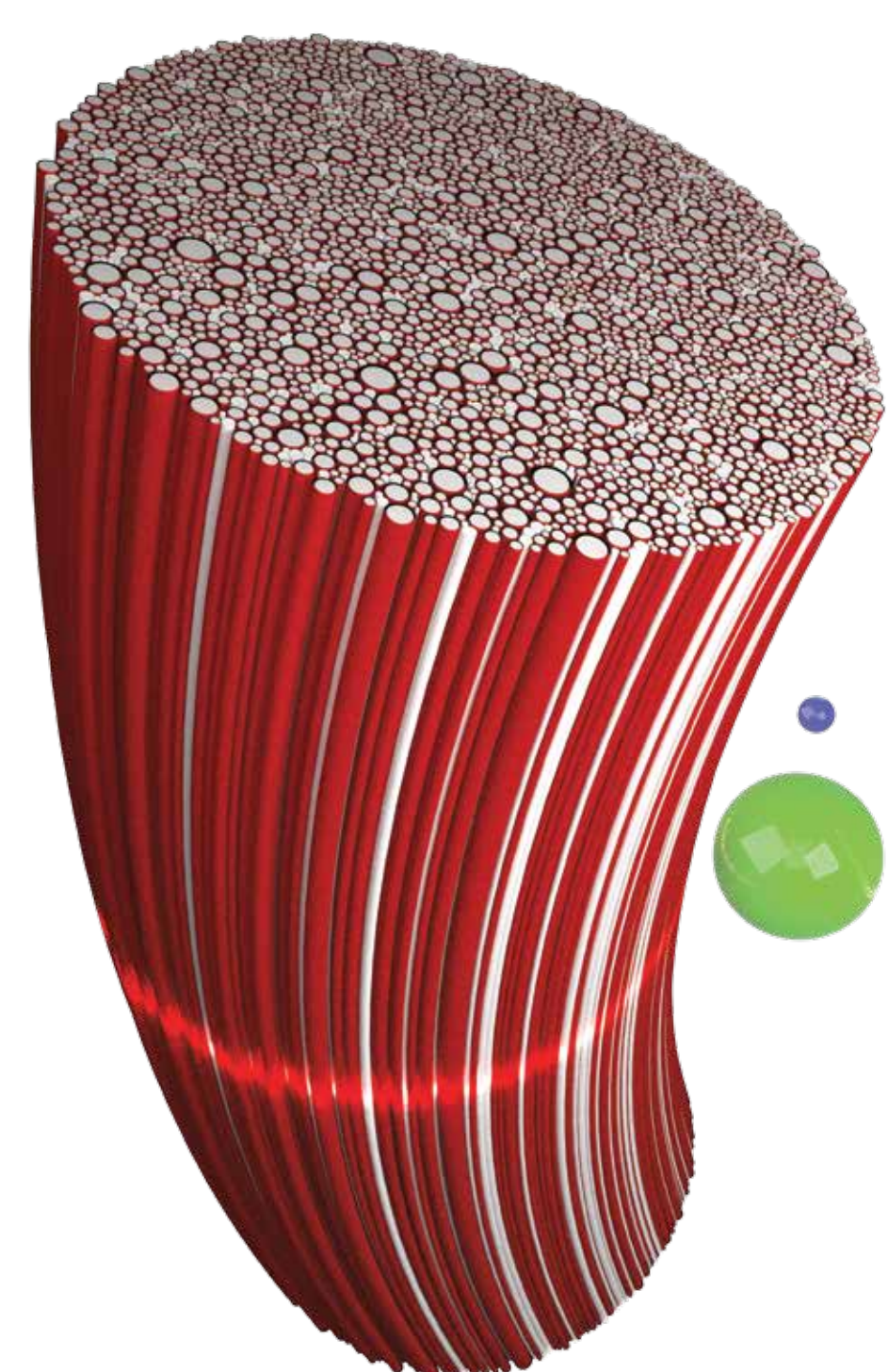
Monte Carlo Diffusion Simulations

- Geometries created with CellBlender: 
 - $L_{\text{axon}} = 160 \mu\text{m}$
 - $d_{\text{axon}} = 3 \mu\text{m}$
- Particle trajectories from MCell (Stiles 1996): 
 - $D = 0.5 \mu\text{m}^2/\text{ms}$
 - $dt = 100 \mu\text{s}$
 - 400000 particles
 - impermeable walls
- dMRI signals calculated with DifSim (Balls 2009):
 - STEAM MR protocol (as above)
 - T2 decay not simulated

Monte Carlo Simulations: Which Factors Might Explain These MR Data?



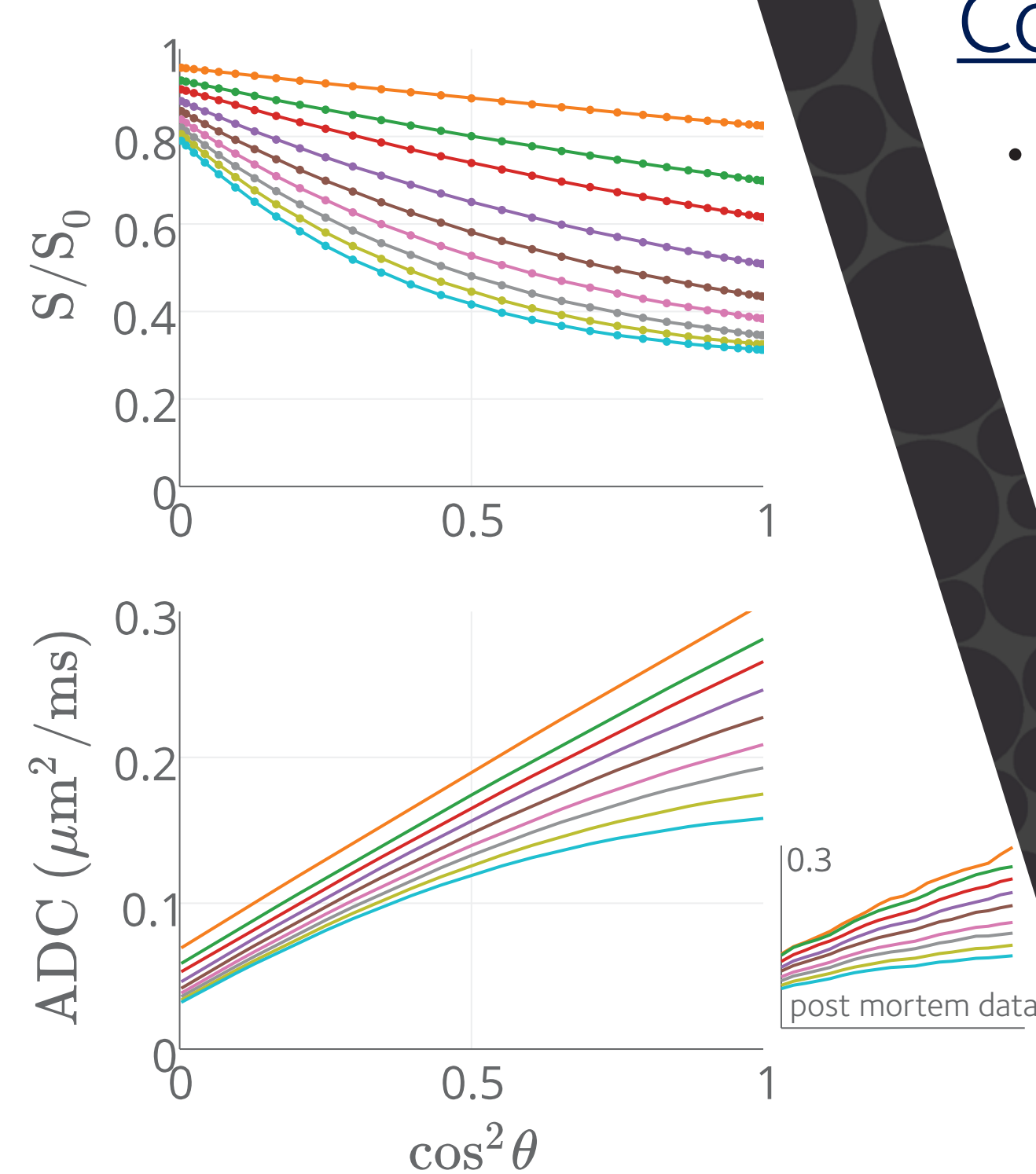
COMBINING FACTORS FOR A BIOPHYSICALLY PLAUSIBLE MODEL



- sensible combination of all of the above approximates the data

MODEL:
gamma-distributed cylinders
 $N=3573$; $\langle \phi \rangle = 0.5 \mu\text{m}$; g-ratio=0.8
bending of 30°
compartments:
25% ECS ($D=5.0 \times 10^{-6} \mu\text{m}^2/\text{ms}$)
10% myelin ($D=1.0 \times 10^{-6} \mu\text{m}^2/\text{ms}$)
40% axons ($D=4.0 \times 10^{-6} \mu\text{m}^2/\text{ms}$)
10% oligodendrocytes ($D=D_{\text{ECS}}$)
10% astrocytes ($D=D_{\text{ECS}}$)
5% mitochondria ($D=1.0 \times 10^{-6} \mu\text{m}^2/\text{ms}$)

- glial volume fractions might still be too high

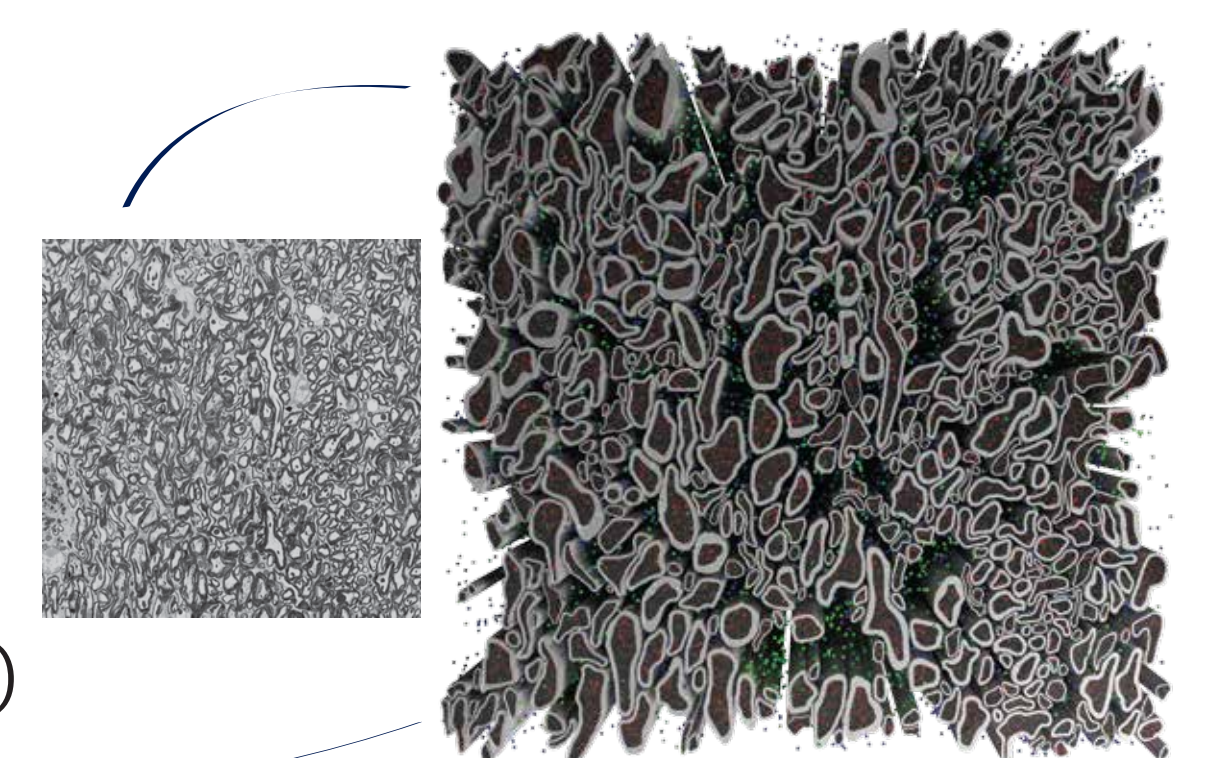


CONCLUSIONS

- The ADC parallel to the bundle is diffusion time dependent
- Monte Carlo simulations suggest the explanation has to involve a combination of microstructural factors
- This work demonstrates a framework for assessing micro structure MRI: from simple cylinders to complex geometry

OUTLOOK: USING EM DATA

- electron microscopy as ground truth for μ -dMRI
- realistic geometries for MC simulations (2D&3D)



RESULTS

CONCLUSION