

ECG Pre-Lab

Sunday, April 23, 2023 1:27 PM

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Original Design:

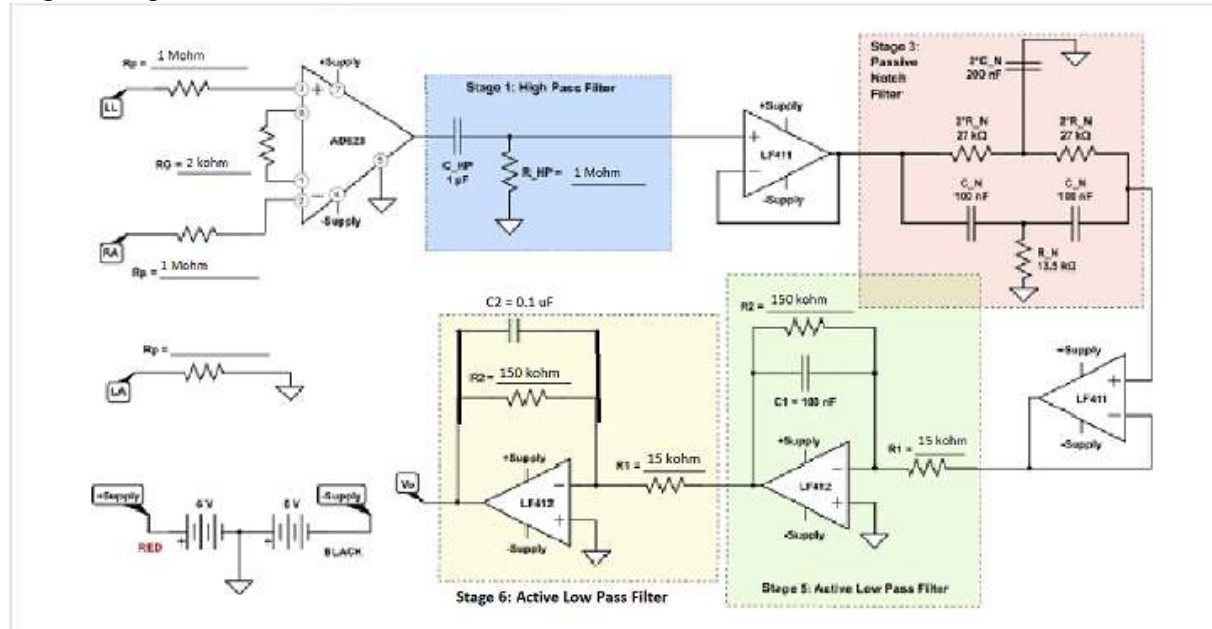


Figure 1: Circuit schematic of Electrocardiogram circuit from EECE 244: Electrocardiogram Circuit Lab handout from

EECE 244: Electrocardiogram Circuit Lab

To provide an additional layer of safety, we will include resistors to limit the maximum current flowing from our circuit to the electrodes. We will employ a factor of safety of 1000; therefore, the maximum current will be limited to $10 \mu\text{A}$. Given a supply voltage of 5V calculate the value of the resistors to achieve a current of $10 \mu\text{A}$.

$$R = \underline{500 \text{ k} \Omega}$$

Round this up to the next resistor available ($100\text{k}\Omega$, $150\text{k}\Omega$, $200\text{k}\Omega$, or $1\text{M}\Omega$)

$$R_p = \underline{1 \text{ M} \Omega}$$

Measurement with an Instrumentation Op Amp

The first stage of amplification uses an AD623 instrumentation amplifier. Locate the formula for setting the gain in the datasheet (<https://www.analog.com/media/en/technical-documentation/data-sheets/ad623.pdf>) and write it below:

$$\text{Gain Formula} = \text{WAVES} \quad 1 + \frac{100 \text{ k}}{R_g}$$

The gain should be between 40 and 60. This will be adjusted later during the tuning phase. Determine an appropriate value for the gain resistor R_g in the circuit shown above.

$$\text{Stage 1 Gain Resistor } R_g = \underline{2 \text{ k} \Omega} \quad (1.7 \text{ k} \rightarrow 2.6 \text{ k}) \Omega$$

$$\text{Gain: } \underline{51}$$

Passive High Pass Filter Design (Stage 1)

We will use a high pass filter to eliminate baseline (DC) drift (e.g. low frequency noise). Generally, the heart rate is above 60 beats per minute (BPM), so we will want to design filter with a f_c below 1 Hz . Given $f_c = 0.16 \text{ Hz}$ and a capacitor $C_{HP} = 1 \mu\text{F}$, calculate the appropriate resistor value for the first-order analog filter used in the ECG circuit.

$$\text{Formula for Cutoff Frequency: } f_c = \frac{1}{2\pi R_{HP} C_{HP}}$$

Given:

$$C_{HP} = 1 \mu\text{F}$$

$$\text{High Pass Frequency } (f_c) = 0.16 \text{ Hz}$$

Find:

$$R_{HP} = \underline{994718 \Omega}$$

Passive Notch Filter Design (Stage 3)

In the second stage or buffer amplifier, we remove 60 Hz noise in stage 3. 60 Hz noise is a particular issue in our electronics lab. This design follows the Twin-T notch topology. Since this design is particularly sensitive to tolerances in component values, you should measure resistances carefully and trim values. The corner frequency (f_c) is found by:

$$f_c = \frac{1}{4\pi R_N C_N}$$

Verify that for the circuit components given in figure 1 that $f_c \approx 60$ Hz. Again, measure component values carefully in this design and match them as well as possible.

Find:

$$f_c = \underline{58.95 \text{ Hz}}$$

Active Low Pass Filter Designs (Stage 5)

Following another buffer (stage 4), is a 1st order active low pass filter. In this design, we want a gain of 10-15 and a low-pass cutoff frequency (f_c) that removes 60 Hz noise and does not overly affect our ECG measurement. Recall that a lower cutoff frequency will provide greater 60 Hz noise attenuation, but too aggressive of a cut-off could lead to signal distortion. Write the formula for the inverting gain and cutoff frequencies (see *Design with Operational Amplifiers and Analog Integrated Circuits* by Sergio Franco, Section 3.2 First Order Active Filters). To design for the gain in the passband, assume that the contributions of the capacitor are negligible (i.e.- the $j\omega C$ term goes to 0).

$$\text{Gain} = -R_2/R_1$$

$$f_c = \frac{1}{2\pi R_2 C_1}$$

Assume the magnitude of the gain is 10 and $f_c = 10.6$ Hz. Use these formulas to select components knowing we'll use: $C_1 = 0.1 \mu\text{F}$. Find R_1 and R_2 .

Given:

$$|\text{Gain}| = 10 \text{ V/V}$$

$$f_c = 10.6 \text{ Hz}$$

Find:

$$R_1 = \underline{15 \text{ k}\Omega}$$

$$R_2 = \underline{150 \text{ k}\Omega}$$

For Stage 6, stage 5 is repeated to further increase the gain of the circuit

Figure 2: EECE 244: Electrocardiogram Circuit Lab handout

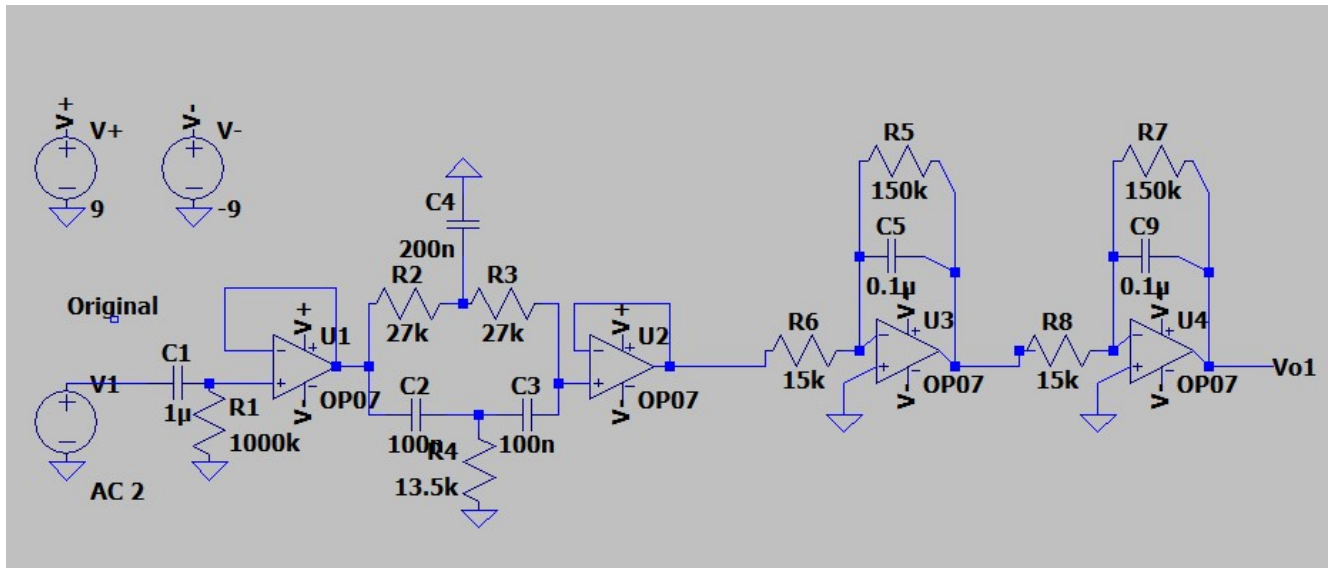


Figure 3: LTSpice Circuit Schematic of stages 1-6 from Figure 1

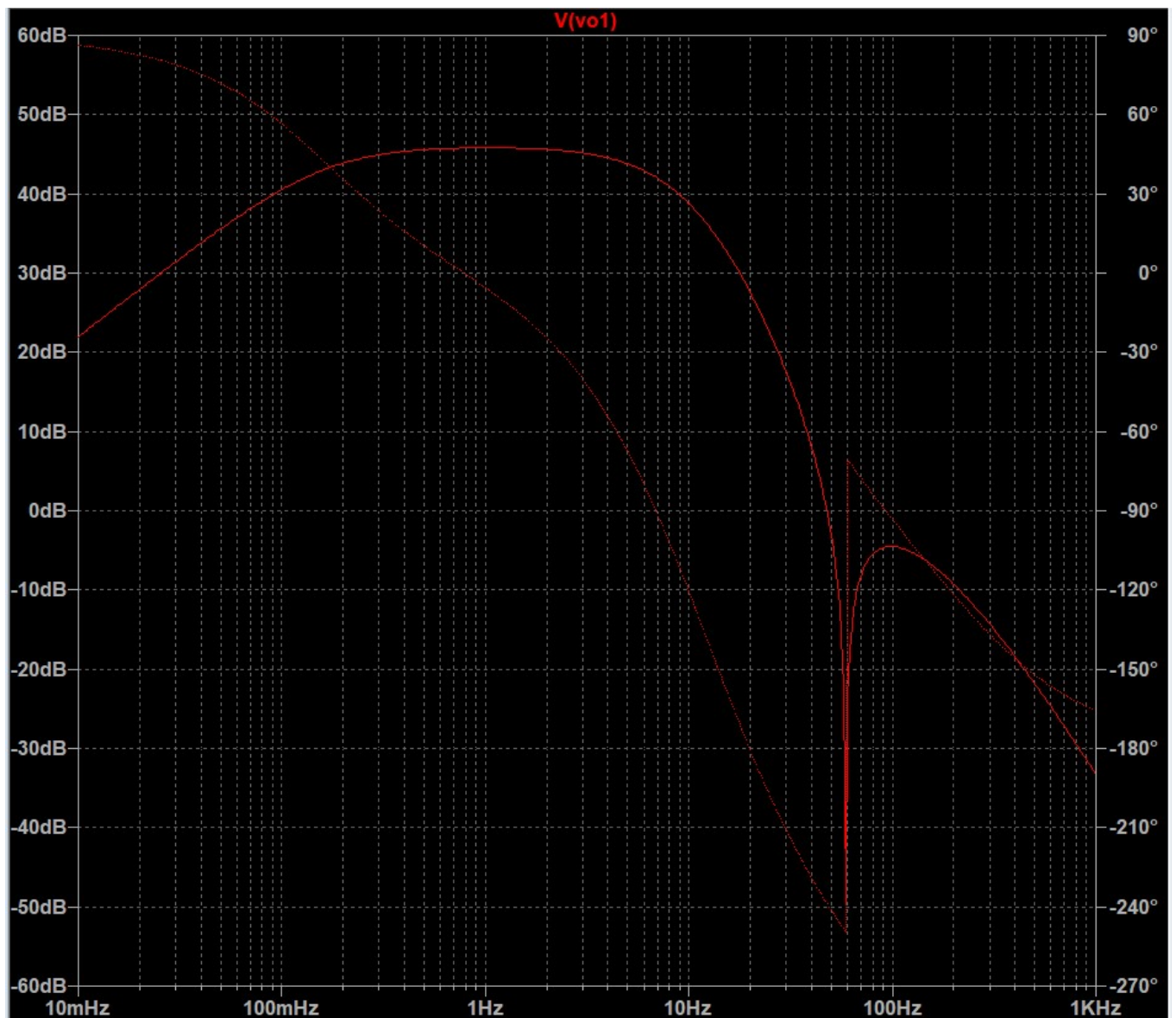


Figure 4: Frequency response of Figure 3 from 0.01Hz to 1KHz at 2 Vpp

Simplified Design:

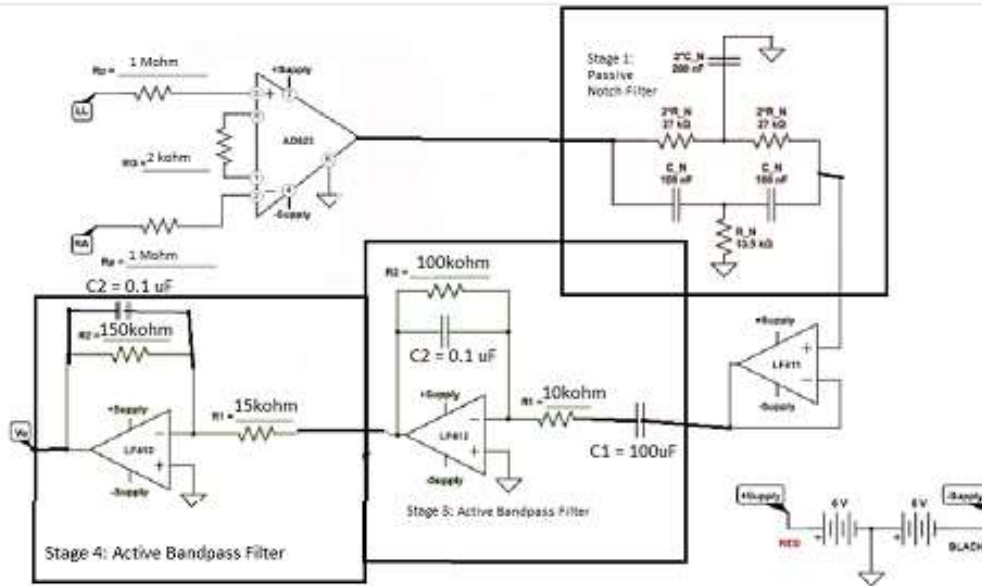


Figure 5: Circuit schematic of Simplified Electrocardiogram circuit

Passive Notch Filter Design (Stage 1)

In the first stage or buffer amplifier, we remove 60 Hz noise in stage 3. 60 Hz noise is a particular issue in our electronics lab. This design follows the Twin-T notch topology. Since this design is particularly sensitive to tolerances in component values, you should measure resistances carefully and trim values. The corner frequency (f_c) is found by:

$$f_c = \frac{1}{4\pi R_N C_N}$$

Verify that for the circuit components given in figure 1 that $f_c \approx 60$ Hz. Again, measure component values carefully in this design and match them as well as possible.

Find:

$$f_c = 68.95 \text{ Hz}$$

Active Band Pass Filter Designs (Stage 3)

In the third stage, we will use an active bandpass filter to eliminate baseline DC drift (e.g. low frequency noise) and 60 Hz noise that does not overly affect our ECG measurement. Generally, the heart rate is above 60 beats per minute (BPM), so we will want to design filter with a f_{c1} below 1 Hz. Recall that a lower cutoff frequency will provide greater 60 Hz noise attenuation, but too aggressive of a cut-off could lead to signal distortion so assume f_{c2} is 10.6 Hz.

Design Equations:

$$f_{c1} = \frac{1}{2\pi R_1 C_1} \quad f_{c2} = \frac{1}{2\pi R_2 C_2}$$

$$\text{Gain} = \frac{-R_2}{R_1}$$

Given:

$$|\text{Gain}| = 10 \frac{V}{V}$$

$$f_{c1} = 0.16 \text{ Hz}$$

$$f_{c2} = 10.6 \text{ Hz}$$

$$C_1 = 10 \mu\text{F}$$

$$C_2 = 15 \mu\text{F}$$

Find

$$R_1 = 100 \text{ k}\Omega$$

$$R_2 = 1 \text{ M}\Omega$$

Using a 1M ohm resistor outside of the instrumentation op amp is not recommended. We also want to try to reduce the capacitor values to maximize slew rate.

To start, R1 will be 100k ohms

For more realistic values:

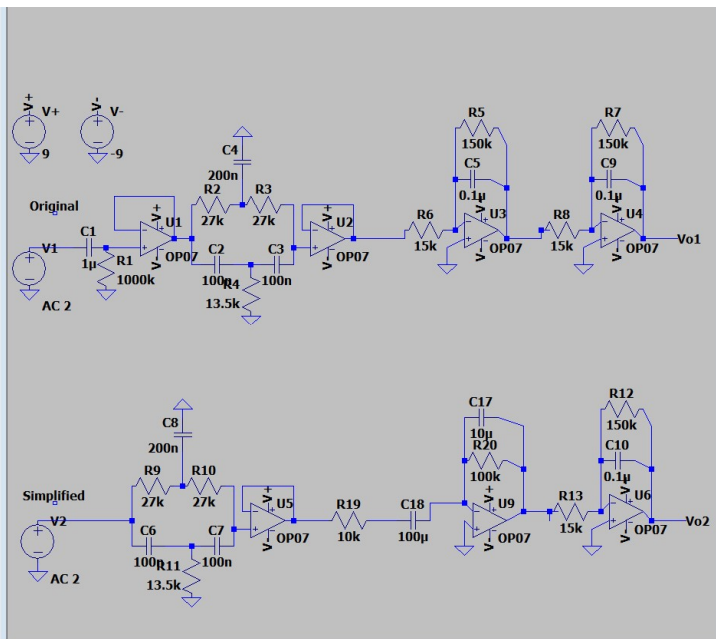
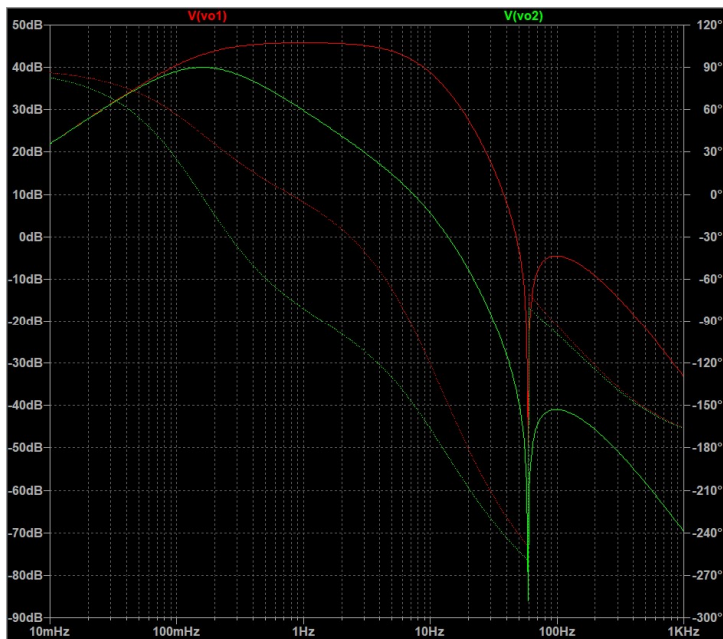
$$R_1 = 10 \text{ k}\Omega$$

$$C_1 = 99 \mu\text{F}_{\text{ideal}} = 100 \mu\text{F}_{\text{standard}}$$

$$R_2 = 100 \text{ k}\Omega$$

$$C_2 = 15 \mu\text{F}_{\text{ideal}} = 10 \mu\text{F}_{\text{standard}}$$

From the calculations above, the bandwidth of the passband is not as large as the bandwidth of the passband in the original circuit.



To fix this, we will set $C_2 = 0.1\mu F$

Active Low Pass Filter Designs (Stage 4)

Following another buffer (stage 4), is a 1st order active low pass filter. In this design, we want a gain of 10-15 and a low-pass cutoff frequency (f_c) that removes 60 Hz noise and does not overly affect our ECG measurement. Recall that a lower cutoff frequency will provide greater 60 Hz noise attenuation, but too aggressive of a cut-off could lead to signal distortion. Write the formula for the inverting gain and cutoff frequencies (see *Design with Operational Amplifiers and Analog Integrated Circuits* by Sergio Franco, Section 3.2 First Order Active Filters). To design for the gain in the passband, assume that the contributions of the capacitor are negligible (i.e.- the $j\omega C$ term goes to 0).

$$\text{Gain} = -R_2/R_1$$

$$f_c = \frac{1}{2\pi R_2 C_1}$$

Assume the magnitude of the gain is 10 and $f_c = 10.6$ Hz. Use these formulas to select components knowing we'll use: $C_1 = 0.1\mu F$. Find R_1 and R_2 .

Given:

$$|\text{Gain}| = 10 \text{ V/V}$$

$$f_c = 10.6 \text{ Hz}$$

Find:

$$R_1 = 15 \text{ k}\Omega$$

$$R_2 = 150 \text{ k}\Omega$$

Figure 6: Design specifications and calculations referring to Figure 5

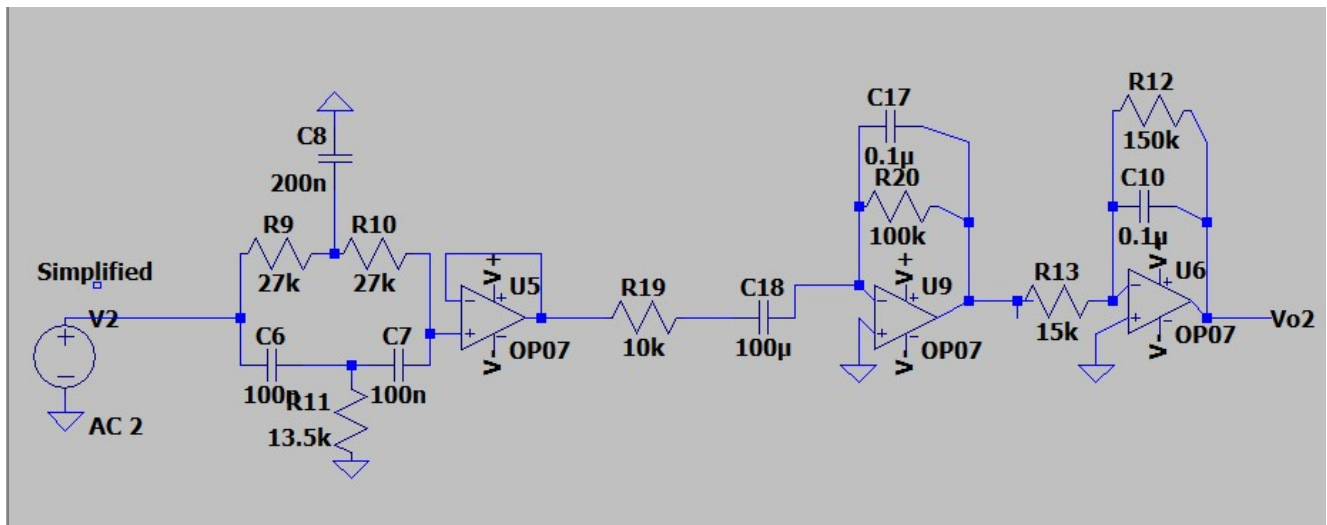


Figure 7: LTSpice Circuit Schematic of stages 1-4 from Figure 5

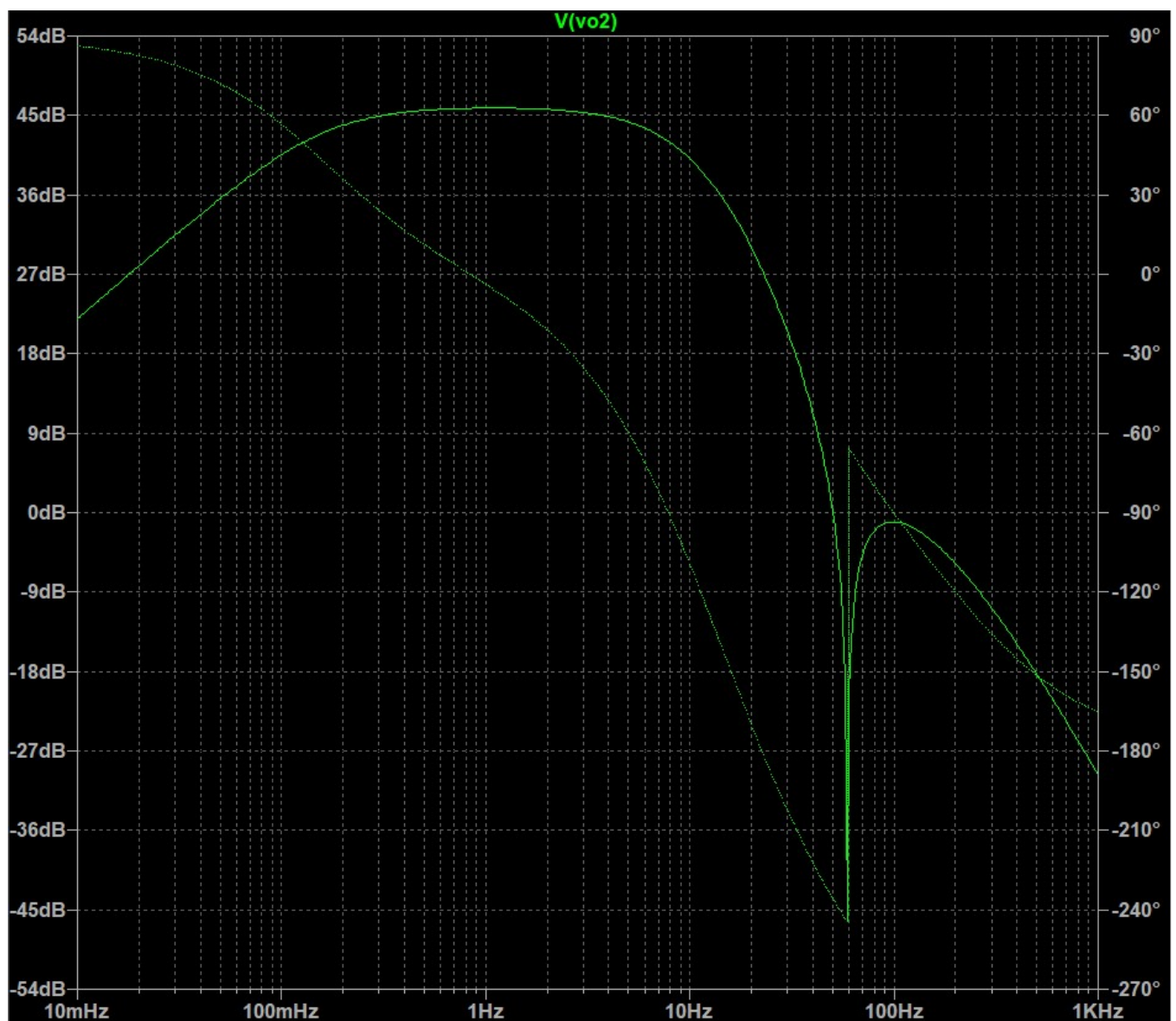


Figure 8: Frequency response of Figure 7 from 0.01Hz to 1KHz at 2 Vpp

Comparison:

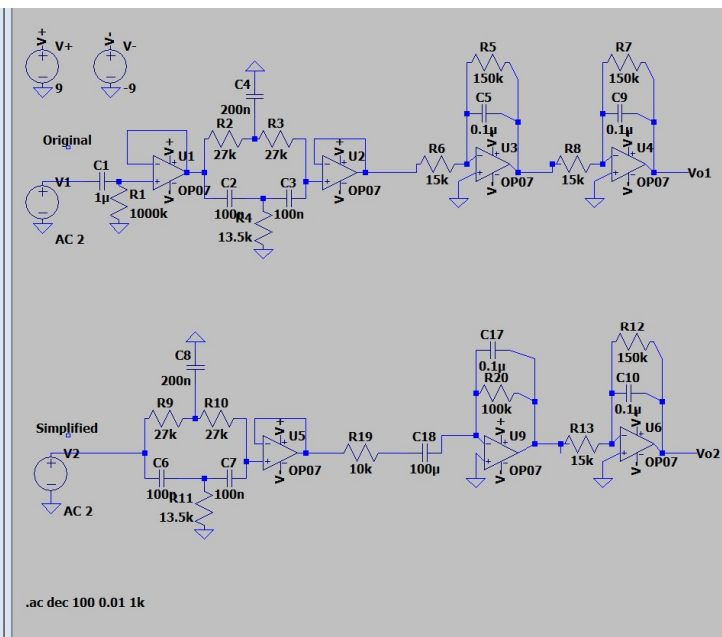
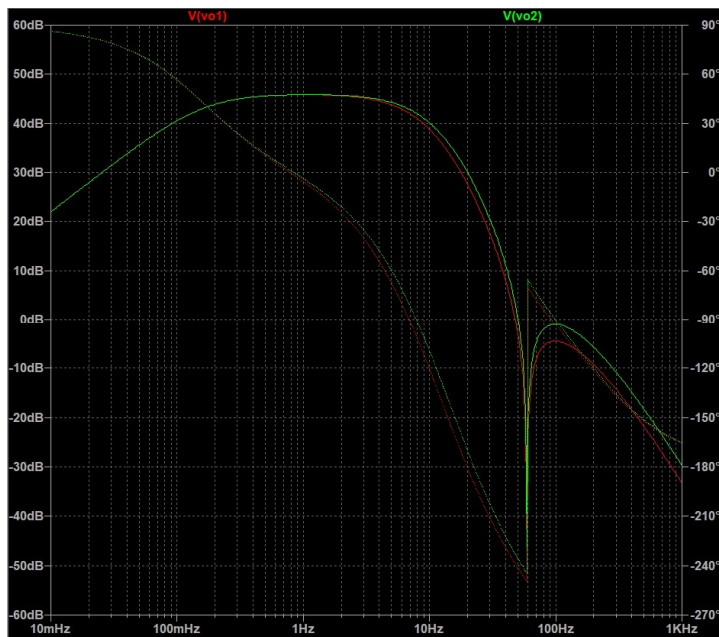


Figure 9: Frequency response comparison of Figure 1 and Figure 7 from 0.01 to 1KHz at 2Vpp

Max Gain = 45.84 dB = 195.9 V/V