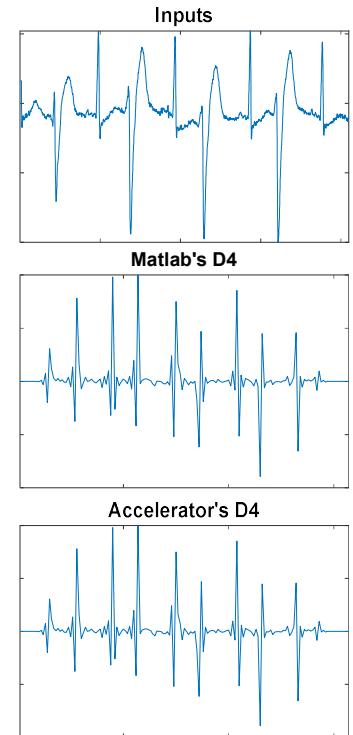


# Design, Implementation, and Verification of a Discrete Wavelet Transform Accelerator Adjacent to AFTAB Microprocessor For Use in Bioelectronic Applications

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## Section 1

# Introduction

*Let your mind fly!*

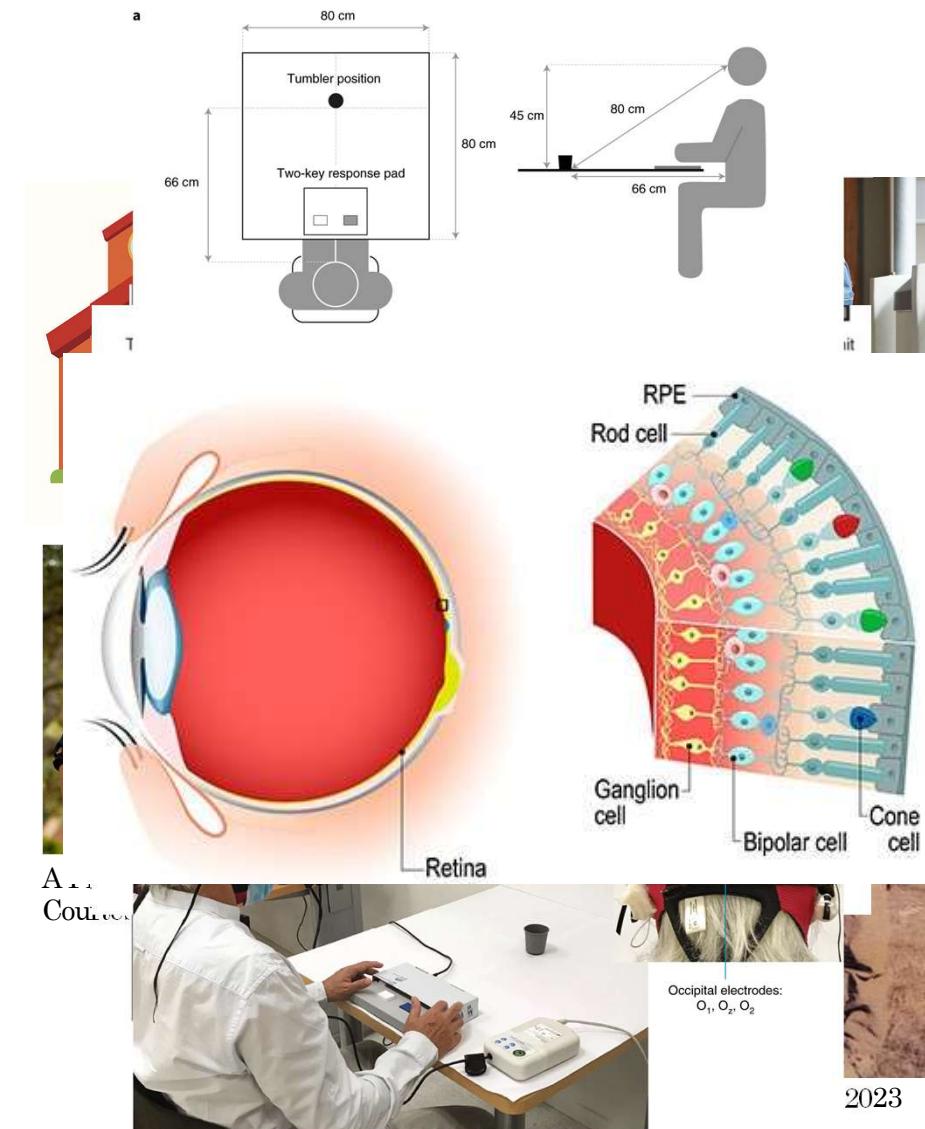
*"Man's mind, once stretched by a new idea, never regains its original dimensions."*

— Oliver Wendell Holmes

# Secular Miracles

## Cure for Blindness, Now Within Sight.

- Restore Vision to the Blind
- Challenges?
  - Pricey!
  - Crude Vision
  - Long Training Cycle
- Alternatives?
  - Give up!
  - Try to Find Better Solutions
- Other Examples
  - Reverse The Effects Of Spinal Cord Injury
  - Brain Interfacing
  - Lab-On-A-Chip
  - Cardiac Pacemakers
  - Cochlear Implants
  - Glucose Monitor
  - Medical Intervention for Epilepsy, Chronic Pain, Parkinson's, Deafness, Essential Tremor



# Motivation. Why Bioelectronics?

- Healthcare And Medicine
- Homeland Security – Bioterrorism
- Forensics
- Protecting The Environment And The Food Supply.

Bottom line

**Key Strategic Drivers**  
**Disease Detection - Disease Prevention - Prosthetics**



➤ Opportunity To Dramatically Increase Synergy Between Electronics And Biology.  
In Monitoring, Processing, and Stimulation.

➤ Potential To Significantly Impact Many Areas Important To the Nation's Economy And The Well-being of its People.

# Semiconductor Technologies

# What Exactly Electronics Offer?

e.g., Cardiac Pacemakers, Sensory Aid Devices

- ❑ Real-time Measurements Decision Making.

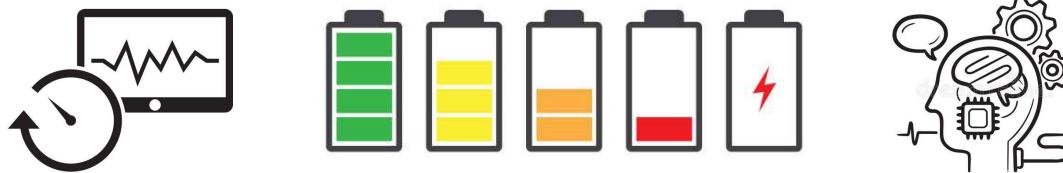
e.g., Nanoscale Bioelectronic Devices  
Integrated with Sensors, Actuators, and Computers

- ❑ Power Savings wherever Possible

e.g., Brain-Computer interfacing.

- ❑ Reduction in the Cost per Unit

- ❑ High-computation Power. High Throughputs.



Bottom line

**There is an opportunity.**  
Utilize the Semiconductor Industry's Capabilities  
Provide Bioelectronic-specific Tools and Systems.

# A Typical Biometrics System.

## 1. Signal Acquisition:

The first step involves the acquisition of signals from biological sources such as electrodes, sensors or stimulation devices.

## 2. Signal Pre-processing:

This stage involves removing noise, filtering, and amplifying the signals to improve the quality of the data.

## 3. Signal Analysis:

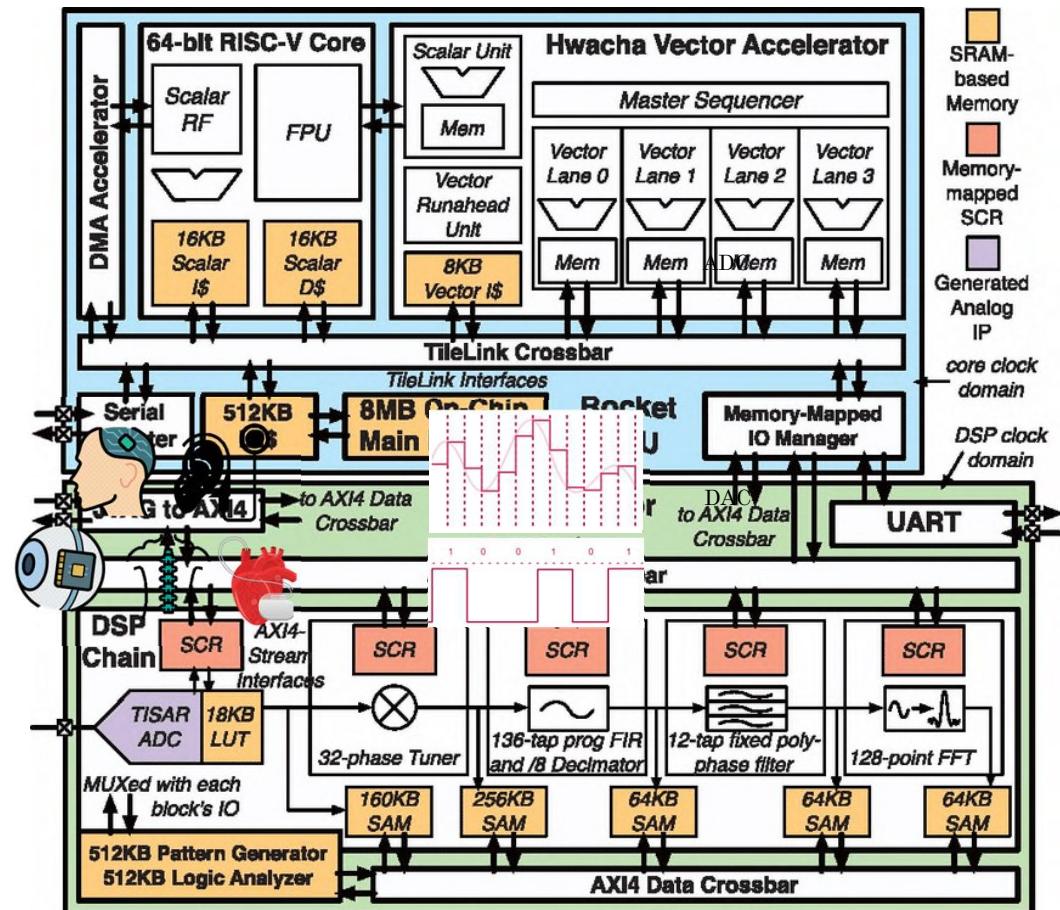
The processed signals are analyzed to extract relevant information, such as detecting specific patterns, calculating measurements or estimating parameters.

## 4. Signal Interpretation:

This stage involves the interpretation of the results obtained from the signal analysis, providing an understanding of the biological processes being monitored.

## 5. Signal Control and Actuation:

In some cases, the processed signals are used to control and actuate devices to influence biological processes.



# How Wavelet Transform Fits.

## 1. WT is a Multi-resolution Analysis.

Time-frequency representation of a signal that provides information about both the location and the magnitude of its frequency components

Why is it important? →

Knowing the timing of a frequency allows for the identification of transient events and changes in the signal that are otherwise difficult to detect using other methods. This information can be used to remove noise and improve the quality of the signal for further analysis and interpretation.

## 2. Effectiveness in Noise Reduction and Compression

Wavelets can concentrate signal energy into a smaller number of coefficients, reducing the amount of data required for storage and analysis.

Why is it important? →

Useful for dimensionality reduction and feature extraction.

## 3. Sparse Representation

Wavelets often provide sparse representations of signals, meaning that most of the information is contained in a small number of coefficients.

## 4. Mathematical Elegance

The wavelet transform has a solid mathematical foundation, which makes it easier to understand, implement, and analyze signals.

Why is it important? →

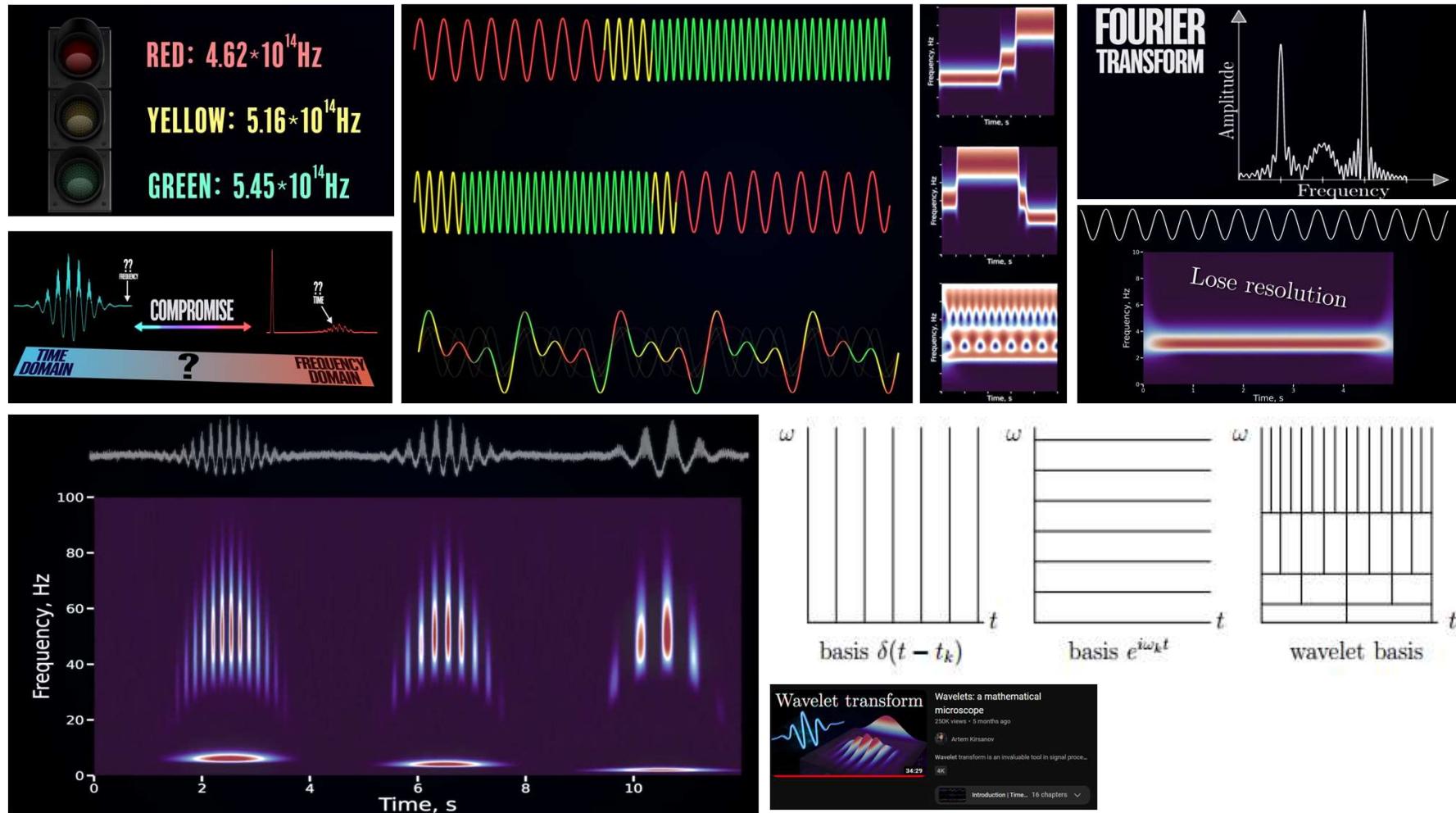
Fourier transform assumes that the signal is stationary, which may not be the case in many real-world signals.

## 5. Handling Non-stationary Signals, and Adaptivity

Wavelet transform is better suited for handling non-stationary signals, where the frequency content of the signal changes over time.

# A Great YouTube Video:

Click here!



# Applications of Wavelet Transform

## 1. Noise Reduction/Removal

Using wavelet thresholding, WT enables us to eliminate the high-frequency noise components without affecting the low-frequency signal components.

## 2. Image Compression

WT decomposes the signals into sub-bands of different frequencies. Each sub-band is then compressed based on its statistical properties, preserving the most important information.

## 3. Quality Assessment

By analyzing the decomposition coefficients, quality assessment metrics such as signal-to-noise ratio, entropy, and energy can be calculated. Can also be used to detect outliers and anomalies, and identify changes in the signal over time

## 4. Data Fusion

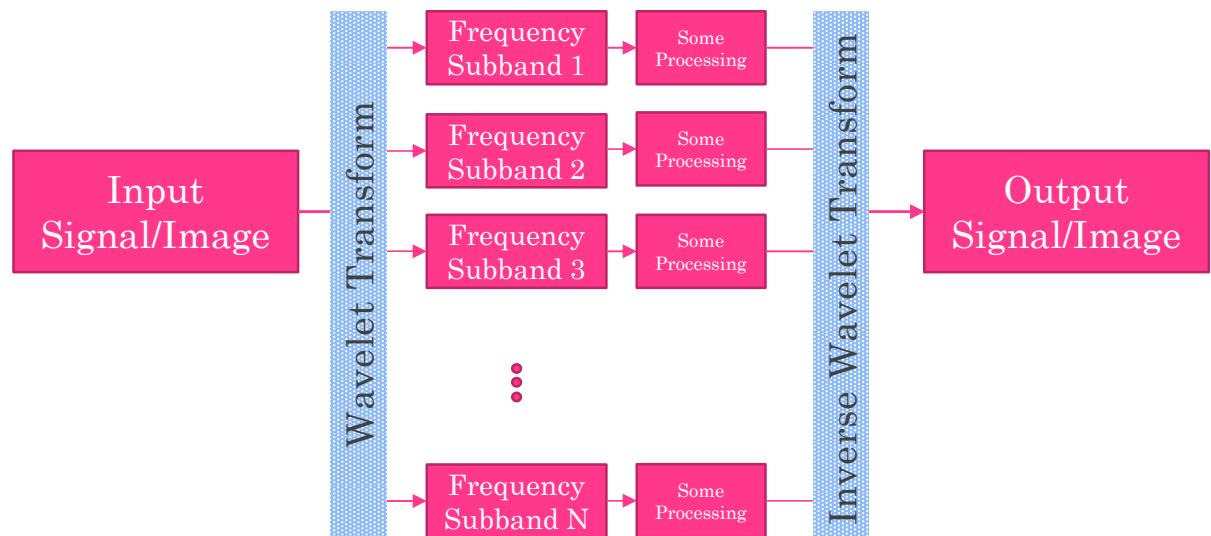
WT is used to combine information from multiple sources, improving the overall quality and reliability of the data. Frequency components can be weighted, based on their relevance or quality, before being recombined into a single signal or image.

## 5. Watermarking

WT is used to embed and detect digital watermarks. Helps ensure the authenticity and integrity of the biomedical signals and images.

## 6. Feature Extraction

WT enables the extraction of important features or patterns at different scales. This information can then be used for various applications, such as classification, diagnosis, or monitoring of medical conditions.



# What is Wavelet Transform?

- Short Answer? A Mathematical Microscope.

- Long Answer?

Continuous WT Mother Wavelets:

$$\psi_{s,\tau}(t) = \frac{1}{\sqrt{s}} \psi\left(\frac{t-\tau}{s}\right)$$

Continuous WT Overarching Equations:

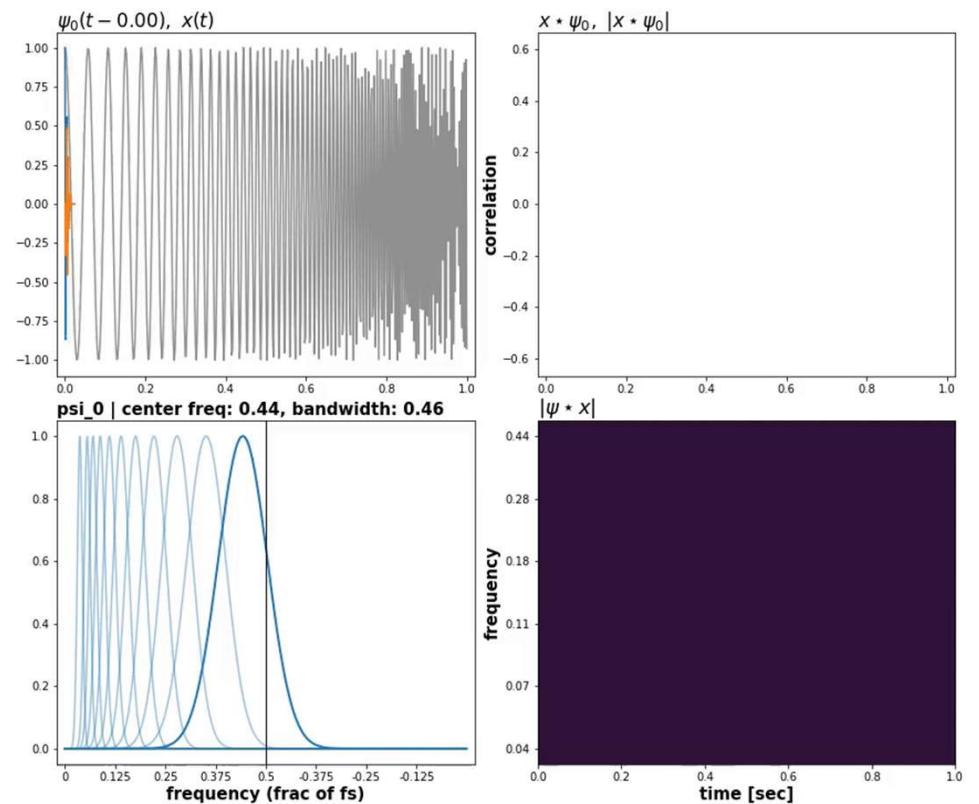
$$\gamma(s, \tau) = \int f(t) \psi_{s,\tau}^*(t) dt \quad f(t) = \int \int \gamma(s, \tau) \psi_{s,\tau}(t) d\tau ds$$

Discrete (Fast) WT Mother Wavelets:

$$\psi_{j,k}(t) = \frac{1}{\sqrt{s_0^j}} \psi\left(\frac{t-k\tau_0 s_0^j}{s_0^j}\right). \quad s_0 = 2, \tau_0 = 1$$

Fourier Property:

$$F\{f(at)\} = \frac{1}{|a|} F\left(\frac{\omega}{a}\right).$$



**Section 2**

# References

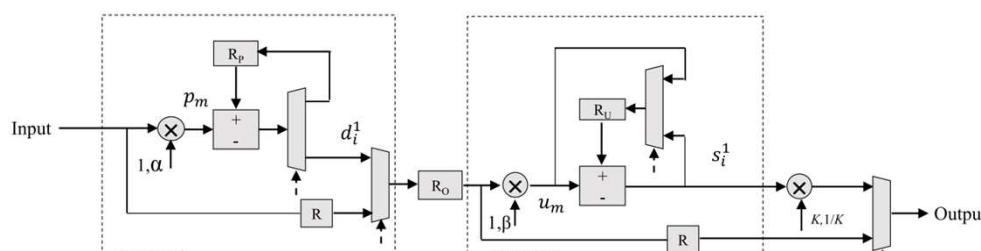
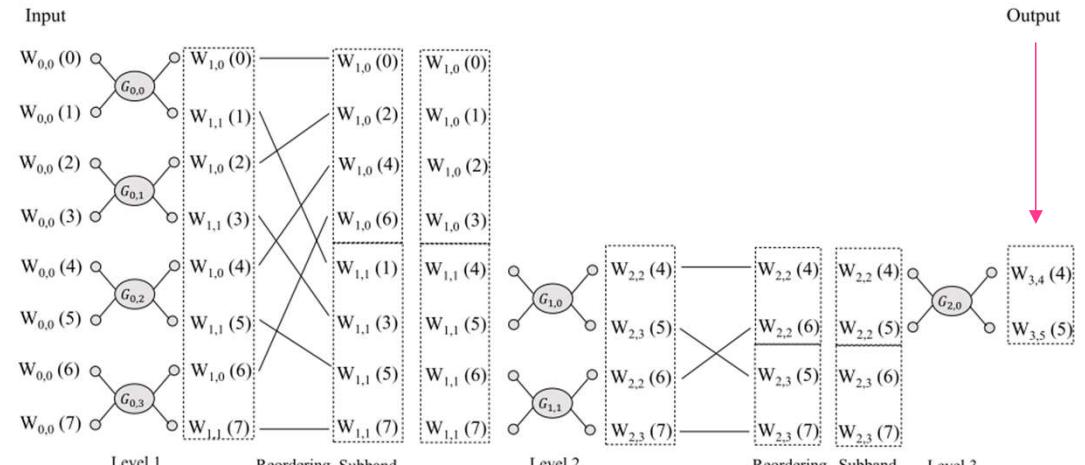
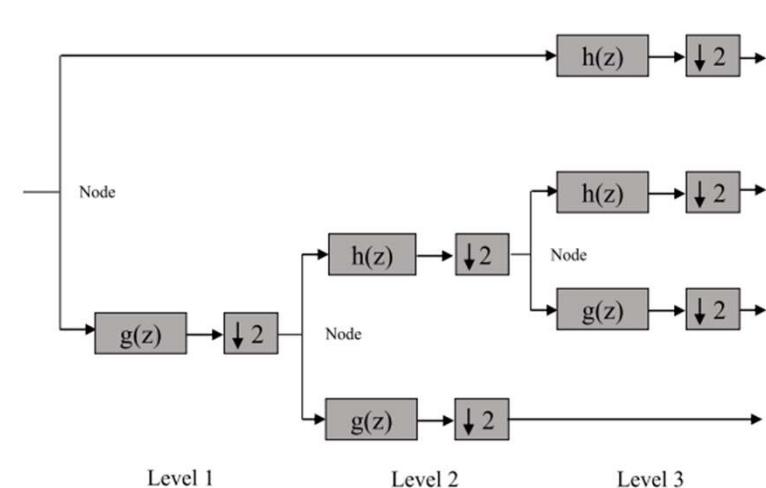
for Future Improvement

# Main References for Future Improvement

- [1] G. Singh, S. R. Chiluveru, B. Raman, M. Tripathy, and B. K. Kaushik, “Novel Architecture for Lifting Discrete Wavelet Packet Transform With Arbitrary Tree Structure,” *IEEE Transactions on Very Large Scale Integration (VLSI) Systems*, vol. 29, no. 7. Institute of Electrical and Electronics Engineers (IEEE), pp. 1490–1494, Jul. 2021. doi: 10.1109/tvlsi.2021.3079989.
- [2] S. A. Salehi and D. D. Dhruba, “Efficient Hardware Implementation of Discrete Wavelet Transform Based on Stochastic Computing,” *2020 IEEE Computer Society Annual Symposium on VLSI (ISVLSI)*. IEEE, Jul. 2020. doi: 10.1109/isvlsi49217.2020.00083.
- [3] M. Tausif, E. Khan, M. Hasan, and M. Reisslein, “Lifting-Based Fractional Wavelet Filter: Energy-Efficient DWT Architecture for Low-Cost Wearable Sensors,” *Advances in Multimedia*, vol. 2020. Hindawi Limited, pp. 1–13, Dec. 16, 2020. doi: 10.1155/2020/8823689.
- [4] R. Pinto and K. Shama, “An Efficient Architecture for Modified Lifting-Based Discrete Wavelet Transform,” *Sensing and Imaging*, vol. 21, no. 1. Springer Science and Business Media LLC, Oct. 26, 2020. doi: 10.1007/s11220-020-00317-z.
- [5] M. Tausif, E. Khan, M. Hasan, and M. Reisslein, “SMFrWF: Segmented Modified Fractional Wavelet Filter: Fast Low-Memory Discrete Wavelet Transform (DWT),” *IEEE Access*, vol. 7. Institute of Electrical and Electronics Engineers (IEEE), pp. 84448–84467, 2019. doi: 10.1109/access.2019.2924490.

# Novel Architecture for Lifting Discrete Wavelet Packet Transform With Arbitrary Tree Structure

G. Singh et al. [2021]

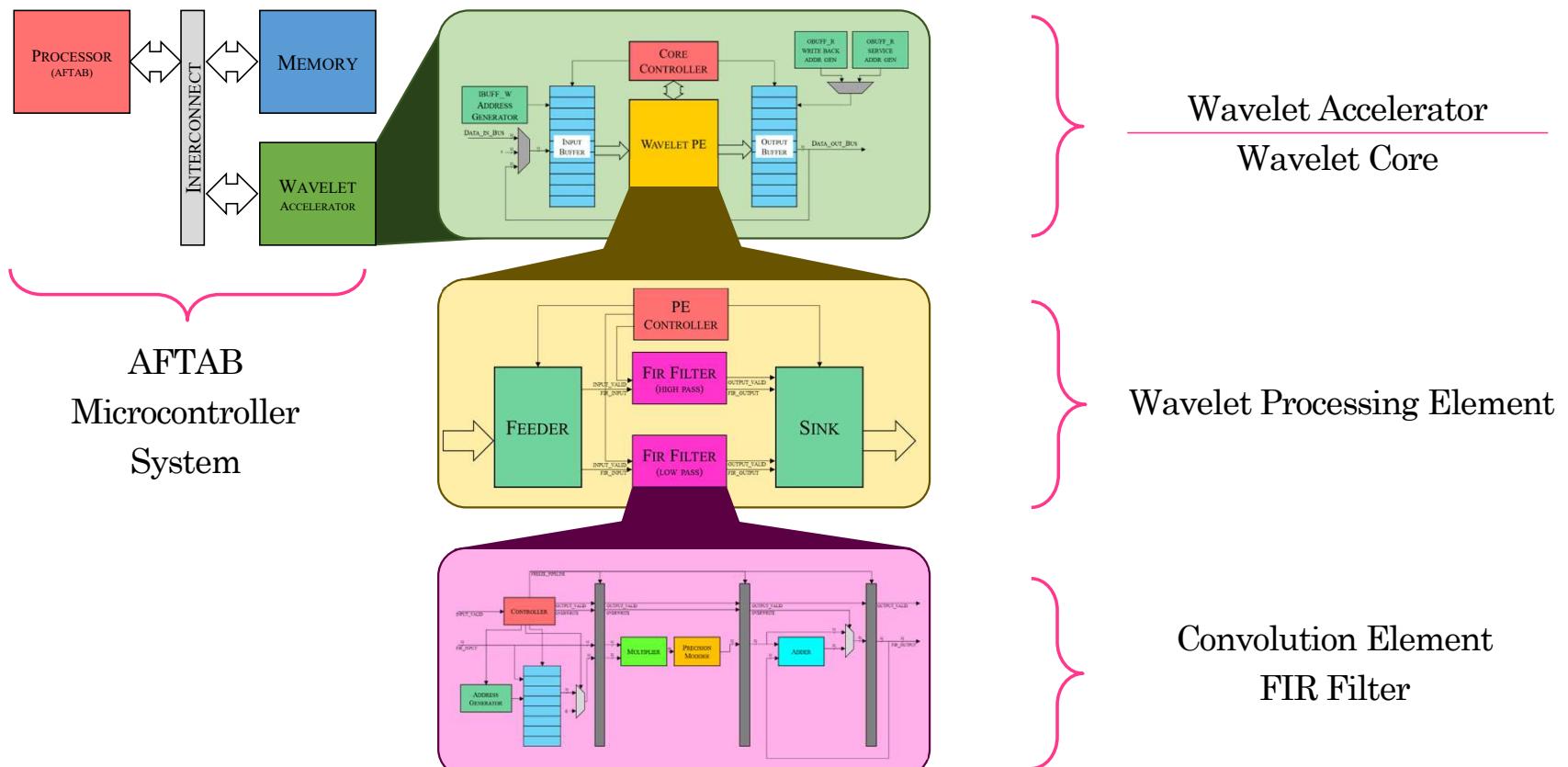


Parameters	Wang et al. [13]	Garcia et al. [14]	This work
Area in $\mu\text{m}^2$ (@90nm)	16255	17327	11622
Power in Watt (@ 250 MHz)	0.0155	0.016	0.013
Gate count	2939	3133	2102

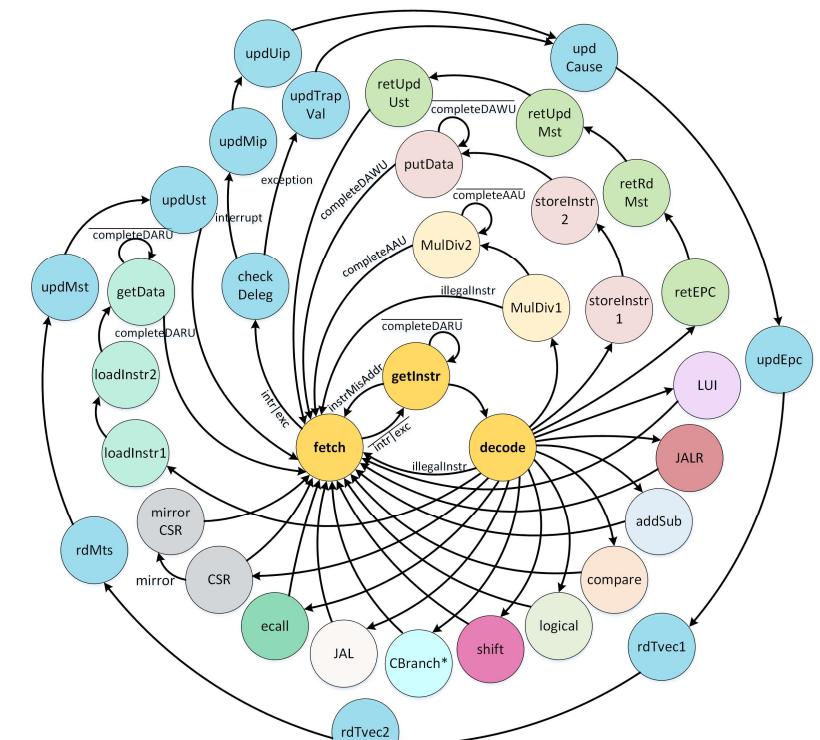
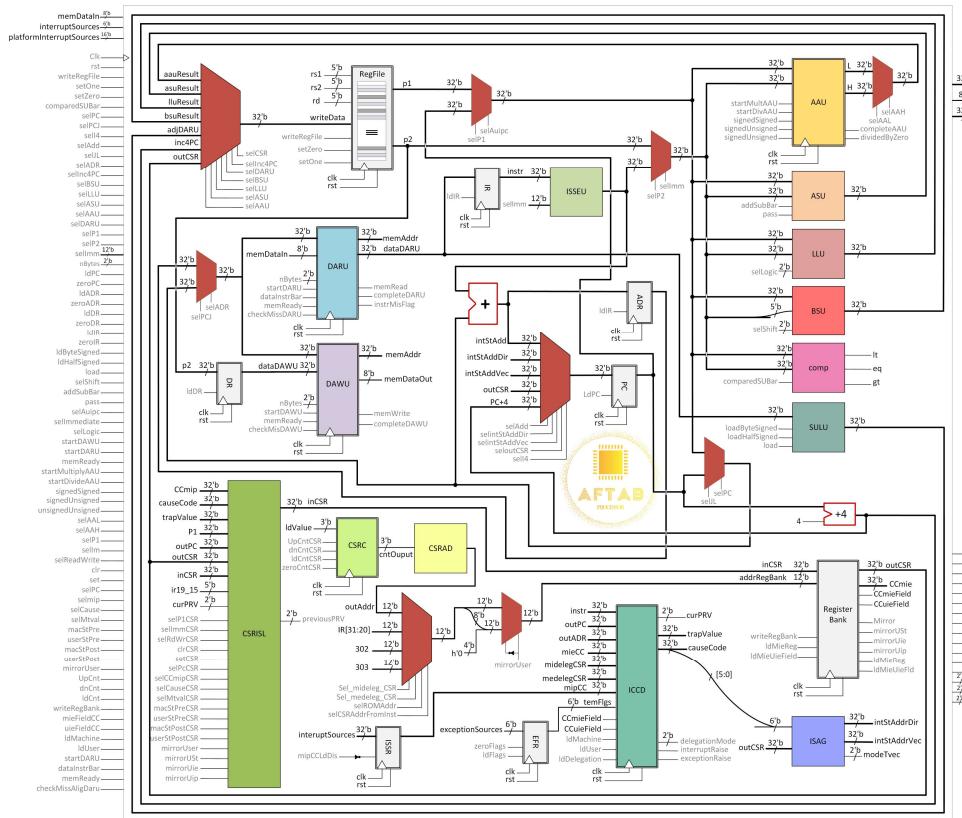
## Section 3

# Accelerator Design

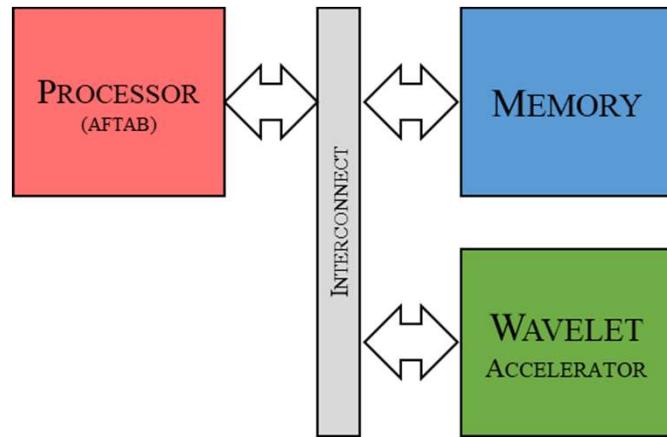
# Bird's Eye View



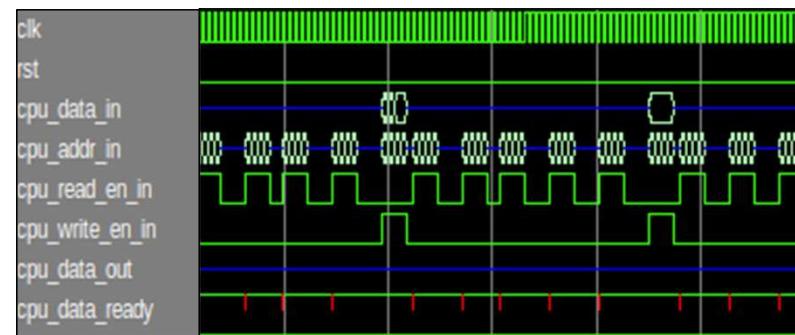
# AFTAB Microcontroller



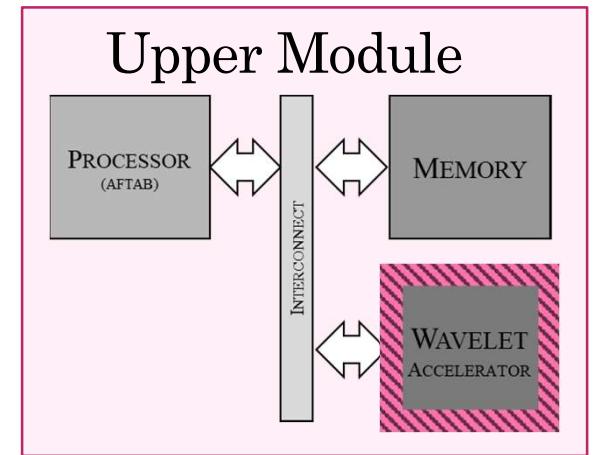
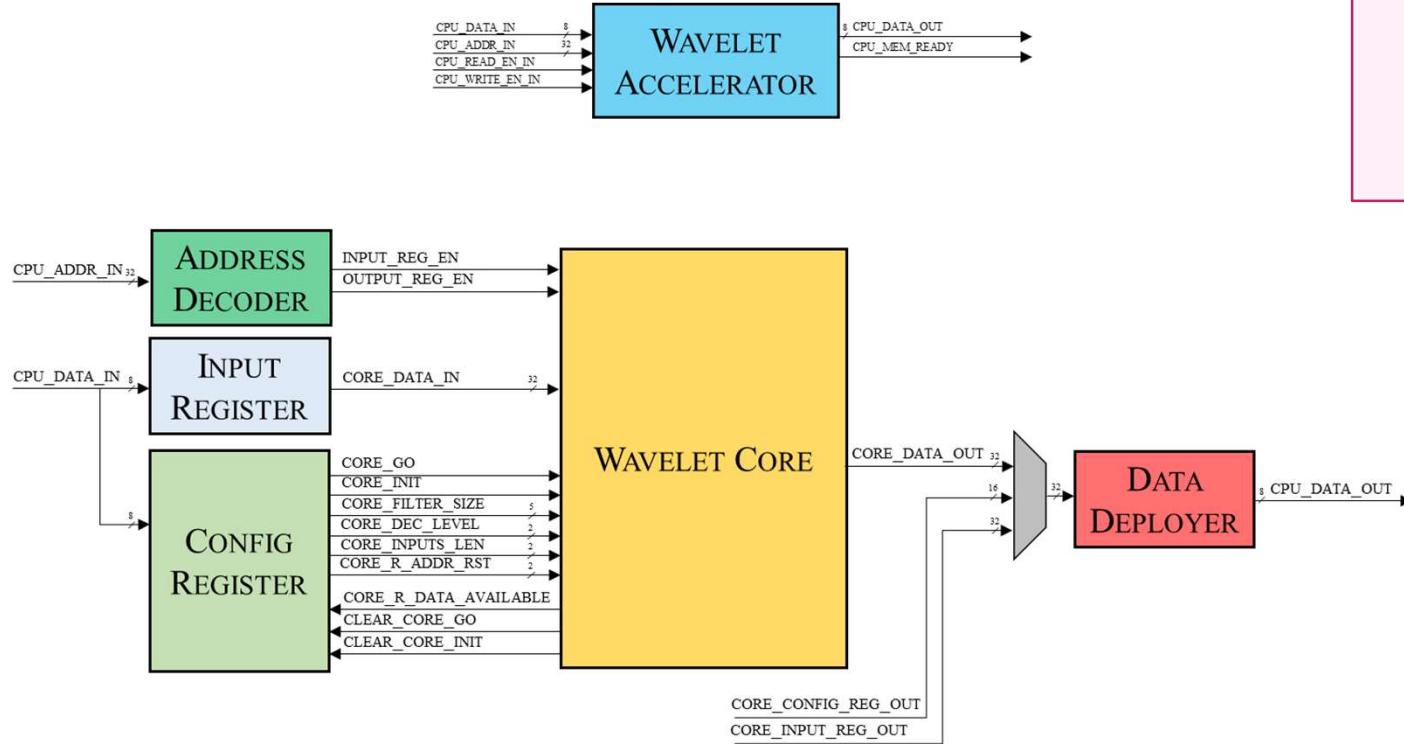
# Accelerator Slave Port



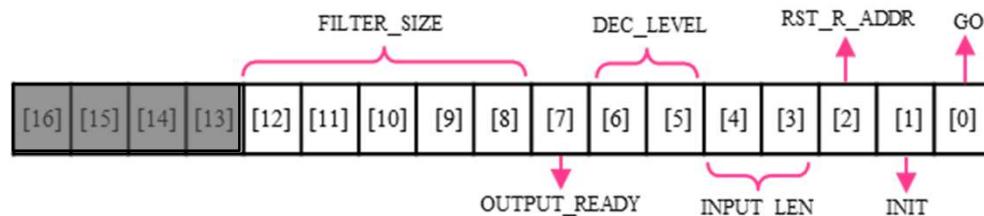
Name	Direction (I/O)	Width
CPU_DATA_IN	Input	8-bits
CPU_ADDRESS_IN	Input	32-bits
CPU_READ_EN_IN	Input	1-bit
CPU_WRITE_EN_IN	Input	1-bit
CPU_DATA_OUT	Output	8-bits
CPU_MEM_READY_OUT	Output	1-bit



# Wavelet Accelerator



# Configuration Register



## 1.GO:

Starts the DWT calculation. Signals the accelerator that the upcoming writes in the Input register are input signal data. After Setting GO, the user's writes to the config register only accept changes to the RST\_R\_ADDR bit. Will be Cleared when the DWT calculation is finished.

## 2.INIT:

Signals the accelerator that the upcoming writes in the Input register are DWT Decomposition Filter Coefficients. After Setting GO, the user's writes to the config register only accept changes to the GO bit. Will be Cleared when FILTER\_SIZE times 2, number of writes to the input register are done.

## 3.RST\_R\_ADDR:

Resets the Pointer to the Output Buffer where the Next Available Output Data is located.

## 4.INPUT\_LEN

Once decoded, determines the number of input signal data.  
 $2'b00 = 256$  samples  
 $2'b01 = 512$  samples  
 $2'b10 = 1024$  samples  
 $2'b11 = 2048$  samples

## 5.DEC\_LEVEL

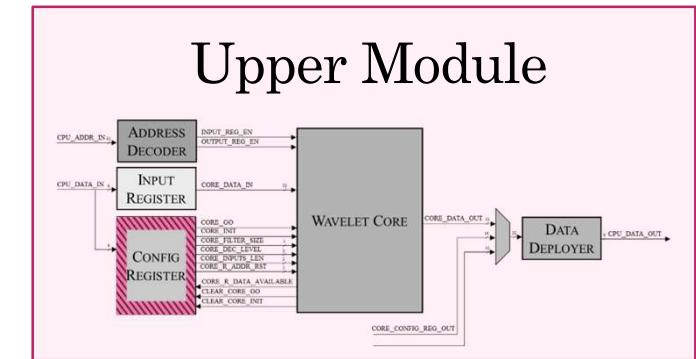
Once Incremented by One, Determines the number of Desired Decomposition Levels.

## 6.OUTPUT\_READY

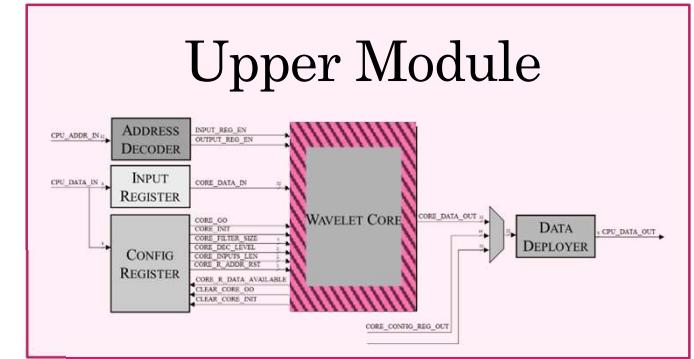
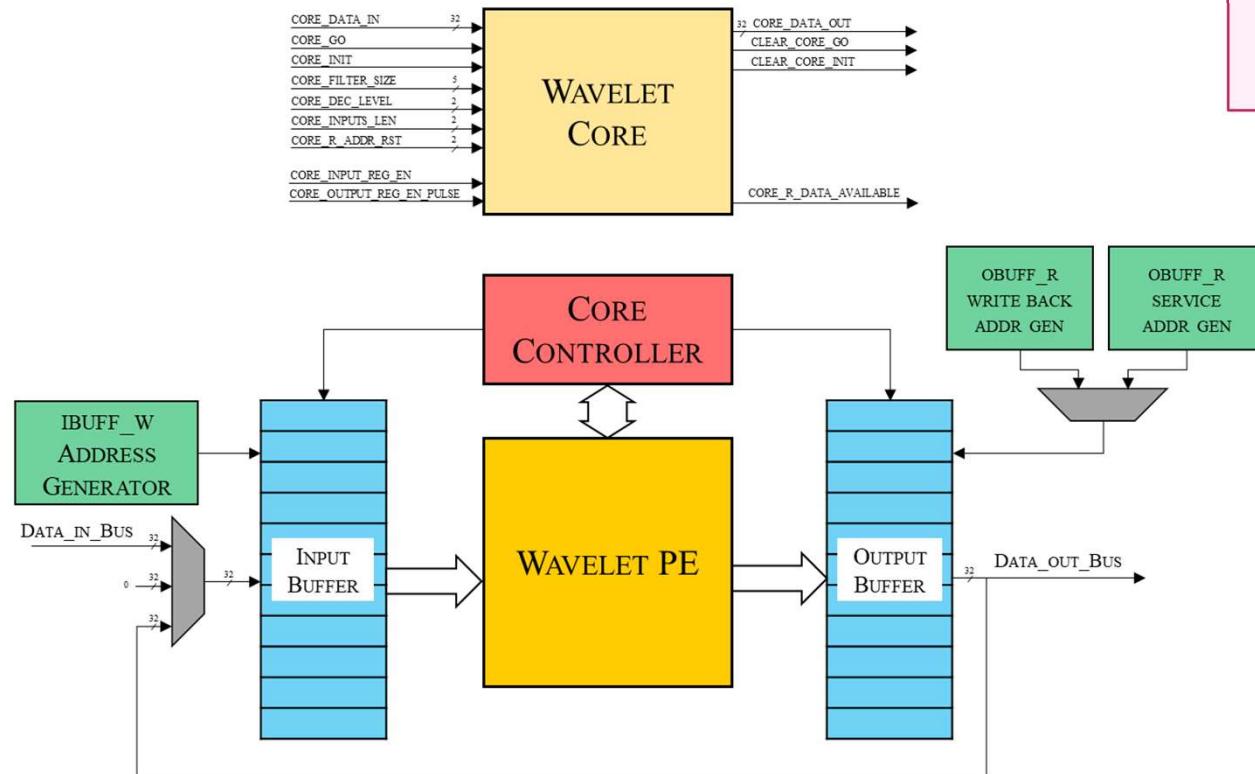
Writes to this bit from the outside are ignored. Once set by core, Conveys there exists unread data in the Output Buffer.

## 7.FILTER\_SIZE:

Once incremented by one, Determines the size of Wavelet Decomposition Filter



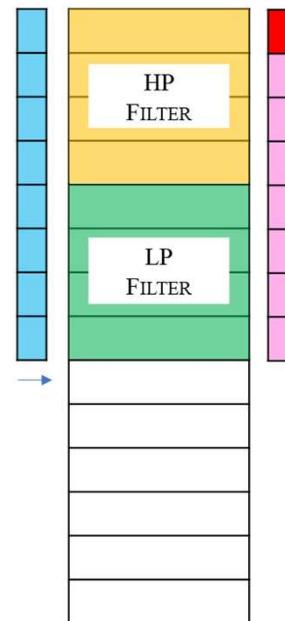
# Wavelet Core



# Input Buffer Wavelet Core

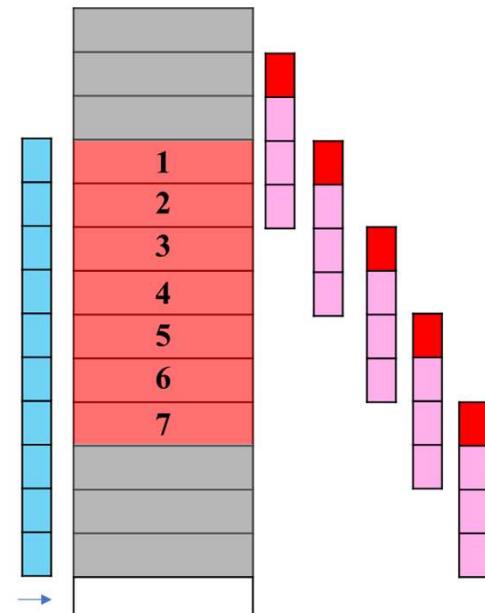
## INPUT BUFFER: INIT

HOW IT'S  
WRITTEN:      HOW IT'S  
READ:

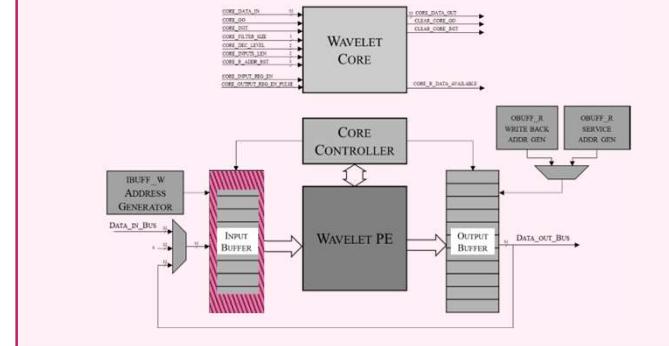


## INPUT BUFFER: GO

HOW IT'S  
WRITTEN:

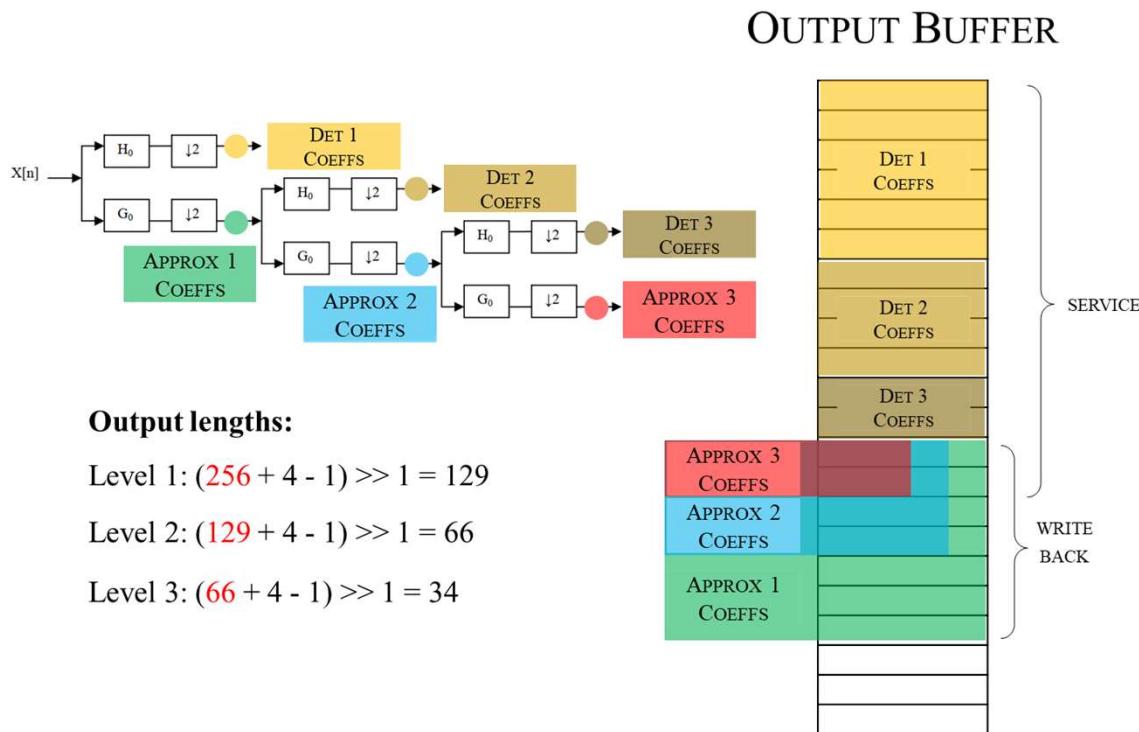


## Upper Module

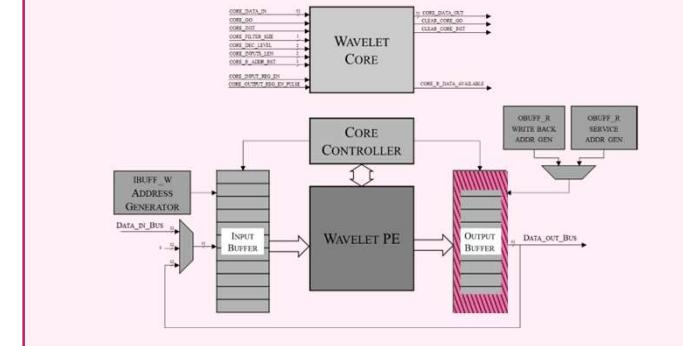


# Output Buffer

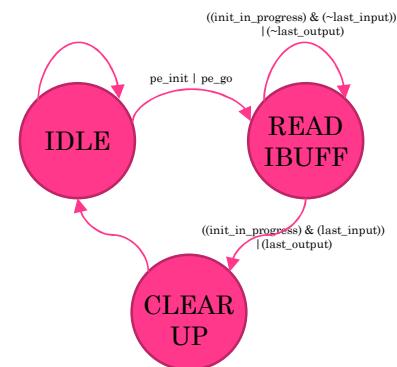
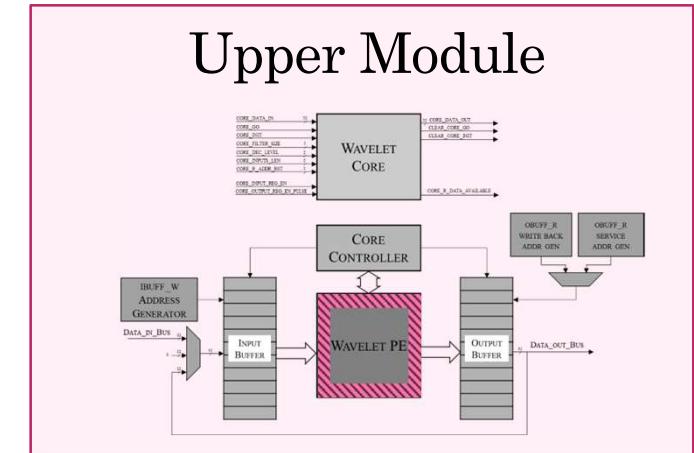
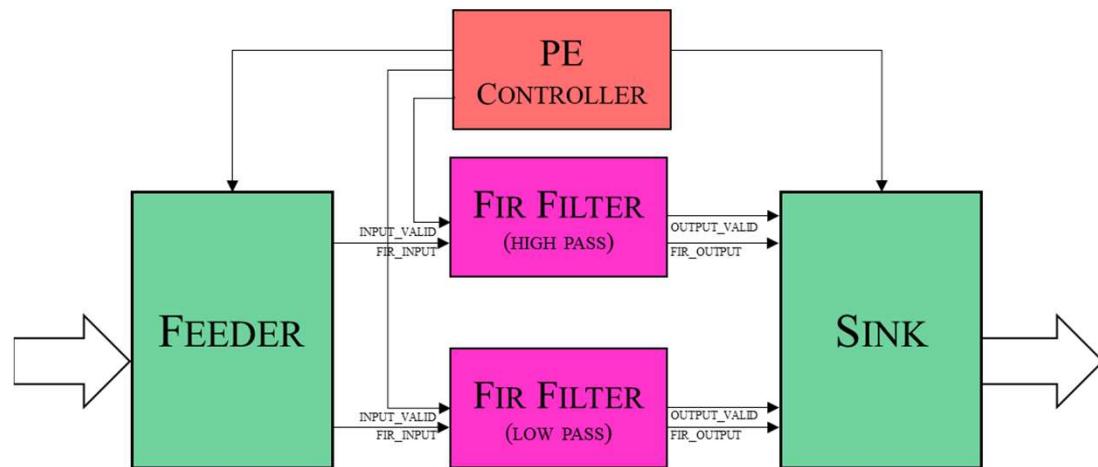
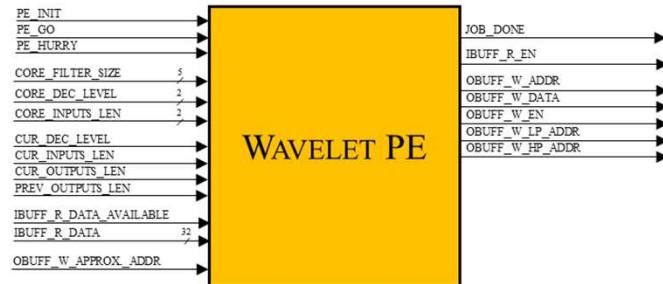
## Wavelet Core



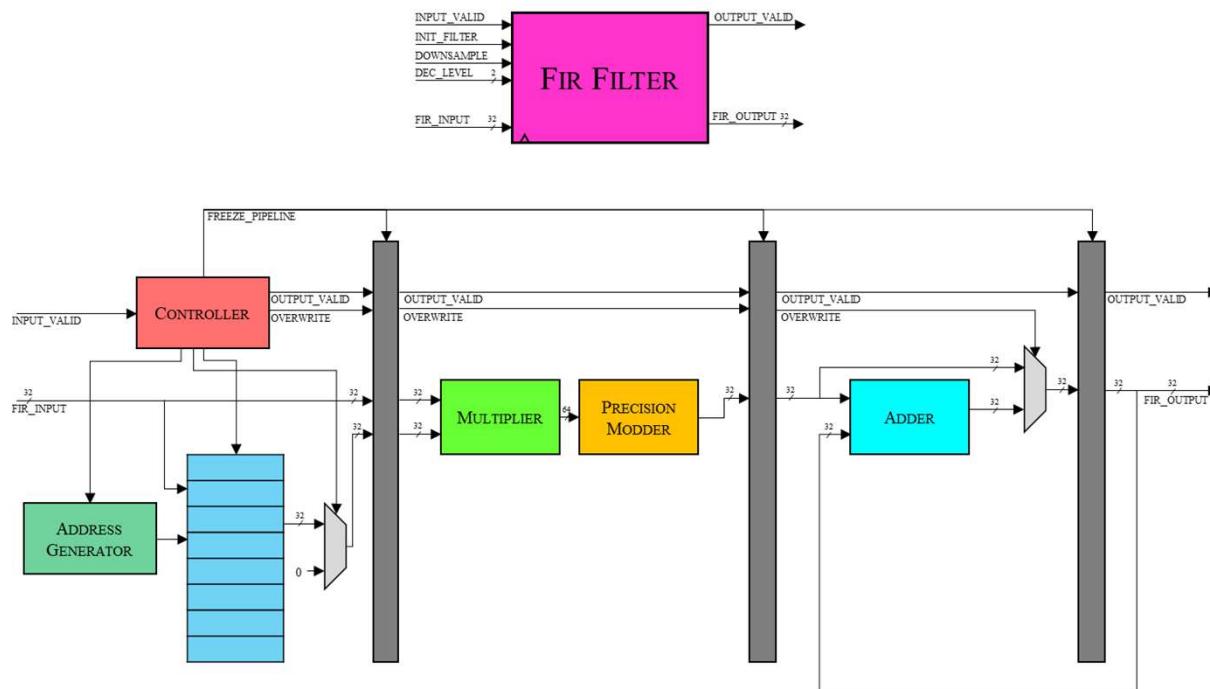
## Upper Module



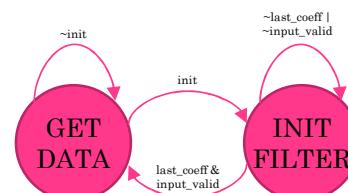
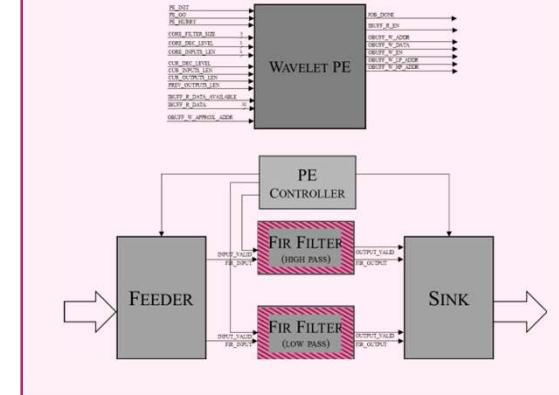
# Wavelet PE



# FIR Filter



Upper Module



## Section 4

# Evaluation

# Evaluation

## Metrics

1. Root Mean Square Error (RMSE) Between MATLAB's Official DWT function, and the Developed Accelerators outputs
2. Speed-up Between Hardware accelerated DWT and Software Implementation of DWT
3. FPGA Resource Usage Before and After Adding the Accelerator
4. Area Comparison on ASIC Before and After Adding the Accelerator

## Actions Taken:

Developed Proprietary 1-D and 2-D DWT function in MATLAB

Developed Proprietary MATLAB to Compare and Display the Results

Developed Testbenches at Various Stages to Mimic AFTAB Behaviour

Developed C Code to Perform and Run DWT Using SW on AFTAB

Performed Synthesis Using Quartus on DE2 FPGA board

Performed ASIC Synthesis and Compared HW Overhead

# RMSE results

[MIT-BIH ECG Arrhythmia Dataset]  
[Max Input Amplitude: 0.1] [FS = 360 Hz]

Test 1				Test 2							
Input Length	Filter Size	Dec Level	Wavelet family	Input Length	Filter Size	Dec Level	Wavelet family				
2048	32	4	Sym16	256	4	1	Db2				
RMS Errors				RMS Errors							
D1	D2	D3	D4	Appr		D1	Appr				
$0.0226e^{-6}$	$0.0227e^{-6}$	$0.0233e^{-6}$	$0.0238e^{-6}$	$0.1501e^{-6}$		$0.2853e^{-8}$	$0.2783e^{-8}$				
Test's Mean RMS Error				Test's Mean RMS Error							
$4.85e^{-8}$				$2.81e^{-9}$							
Mean RMS Error											
$2.56e^{-8}$											

# Speed-up results

Test 1				Test 2											
Input Length	Filter Size	Dec Level	Wavelet family	Input Length	Filter Size	Dec Level	Wavelet family								
2048	32	4	Sym16	256	4	1	Db2								
HW Accelerated Runtime		Software Runtime		HW Accelerated Runtime		Software Runtime									
768,760 ns		$\approx 119,919,936$ ns		635,620 ns		14,594,030 ns									
Test's Speed-up				Test's Speed-up											
159.9				22.9											
Mean Speed-up															
91.4															

# FPGA Resource Usage and FMAX

DE2 Cyclone II EP2C35F672C6	
Combinational Function	Logic Registers
1,556 / 33,216 (5%)	456 / 33,216 (1%)
Total Logic Elements	
1,619 / 33,216 (5%)	
Total Memory Bits	
264,192 / 483,840 (55%)	
Embedded 9-bit Multiplier elements	
16 / 70 (13%)	

DE2 Cyclone II EP2C35F672C6
FMAX
61.36 MHz

## Accelerator Testbench

```

344 initial begin
345     clk          = 0;
346     rst          = 0;
347     cpu_data_in  = {(8){1'b0}};
348     cpu_addr_in  = {(32){1'b0}};
349     cpu_read_en_in = 0;
350     cpu_write_en_in = 0;
351     filter_size   = FILTER_SIZE - 1;
352     inputs_len    = INPUTS_LEN;
353     dec_level     = DEC_LEVEL - 1;
354
355     duv_system_reset();
356
357     duv_put_configs();
358
359     duv_put_init();
360
361     duv_put_coeffs();
362
363     duv_wait_init_finish();
364
365     duv_put_go();
366
367     duv_reset_r_addr();
368
369     duv_put_signal();
370
371     duv_wait_go_finish();
372
373     duv_read_outputs();
374
375     repeat(100) @ (posedge clk);
376     $stop();
377 end
378
379 endmodule

```

## DWT Using Hardware

```

280 int main()
281 {
282     // duv_put_configs
283     *((int*)0x1A100000) = 0x0300; //000_00011_0_00_00_0_0_0;
284
285     // duv_put_init
286     *((int*)0x1A100000) = 0x0302; //000_00011_0_00_00_0_1_0;
287
288     // duv_put_coeffs
289     *((int*)0x1A100004) = 0xC22E4571;
290     *((int*)0x1A100004) = 0x6B12F75B;
291     *((int*)0x1A100004) = 0xE34F40F4;
292     *((int*)0x1A100004) = 0xEF6FB23E;
293
294     *((int*)0x1A100004) = 0xEF6FB23E;
295     *((int*)0x1A100004) = 0x1CB0BF0B;
296     *((int*)0x1A100004) = 0x6B12F75B;
297     *((int*)0x1A100004) = 0x3DD1BA8E;
298
299
300     // duv_wait_init_finish
301     while((*((int*)0x1A100000) & 0x0002)) {}
302
303     // duv_put_go
304     *((int*)0x1A100000) = 0x0301;
305
306     // duv_reset_r_addr
307     *((int*)0x1A100000) = 0x0306;
308
309     // duv_put_signal
310     int input_idx;
311     for(input_idx = 0; input_idx < 256; input_idx = input_idx + 1) {
312         *((int*)0x1A100004) = test_inputs[input_idx];
313     }
314
315     // duv_read_outputs
316     int output_idx = 0;
317     int output_data;
318     while(1) {
319         while(!((int*)0x1A100000) & 0x0008)) {}
320         output_data = *((int*)0x1A100008);
321         output_idx = output_idx + 1;
322         if(output_idx == 258)
323             break;
324     }
325
326     return 0;
327 }

```

## DWT Using Software

```

void apply_filter(int* filtered_signal, int input_signal[], unsigned int input_length, int filter_bank[], unsigned int filter_length) {
    int* signal_window = (int*) 0x00100408;
    unsigned int edge_index;

    for(edge_index = 1; edge_index < (input_length+filter_length); edge_index = edge_index + 2) {
        signal_window[0] = input_signal[edge_index];
        signal_window[1] = input_signal[edge_index-1];
        int tmp = 0; unsigned int i;
        for(i = 0; i < filter_length; i = i + 1) {
            tmp = tmp + signal_window[i] * filter_bank[i];
        }
        filtered_signal[edge_index] = tmp;
        for(i = filter_length - 1; i >= 1; i = i - 1) {
            signal_window[i] = signal_window[i-1];
        }
        for(i = filter_length - 1; i >= 1; i = i - 1) {
            signal_window[i] = signal_window[i-1];
        }
    }
    return;
}

void wavelet_analysis(int* dwt_coeff, int decomposition_level,
                     unsigned int signal_length, unsigned int filter_length) {
    int* cur_inputs = &test_inputs[0];
    int* detail_coeff = (int*) 0x00100200;
    int* approx_coeff = (int*) 0x00100300;
    int dec_idx; unsigned int i; unsigned int coeffs_length; unsigned int prev_coeff = 0;

    int cur_inputs_length = signal_length;
    for(dec_idx = 0; dec_idx < decomposition_level; dec_idx = dec_idx + 1) {
        apply_filter(dwt_coeff, cur_inputs, cur_inputs_length, hid_coeff, filter_length);
        coeffs_length = ((cur_inputs_length + filter_length - 1) >> 1);
        for(i = 0; i < coeffs_length; i = i + 1) {
            dwt_coeff[prev_coeff+i] = detail_coeff[i];
        }

        apply_filter(approx_coeff, cur_inputs, cur_inputs_length, lod_coeff, filter_length);
        prev_coeff = prev_coeff + coeffs_length;
        for(i = 0; i < coeffs_length; i = i + 1) {
            cur_inputs[i] = approx_coeff[i];
        }

        cur_inputs_length = coeffs_length;
    }

    for(i = 0; i < coeffs_length; i = i + 1) {
        dwt_coeff[prev_coeff+i] = approx_coeff[i];
    }
}

```

## Section 5

# Conclusion

# Looking Back ...

## 1. Signal Acquisition:

The first step involves the acquisition of signals from biological sources such as electrodes, sensors or stimulation devices.

## 2. Signal Pre-processing:

This stage involves removing noise, filtering, and amplifying the signals to improve the quality of the data.

## 3. Signal Analysis:

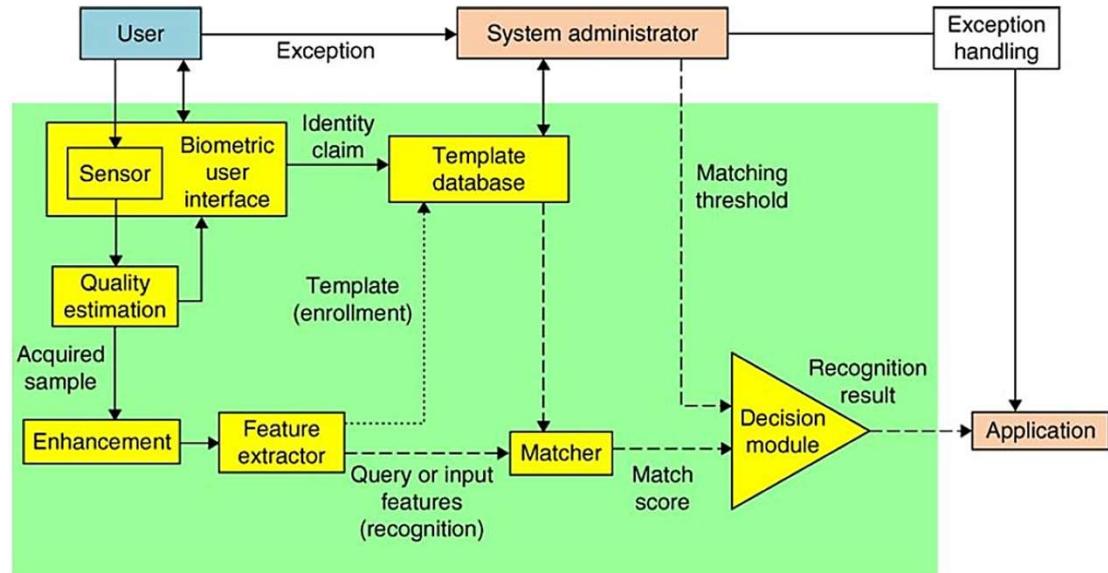
The processed signals are analyzed to extract relevant information, such as detecting specific patterns, calculating measurements or estimating parameters.

## 4. Signal Interpretation:

This stage involves the interpretation of the results obtained from the signal analysis, providing an understanding of the biological processes being monitored.

## 5. Signal Control and Actuation:

In some cases, the processed signals are used to control and actuate devices to influence biological processes.



# What's been Achieved.

Mean Speed-up	Mean RMS Error
91.4	$2.56e^{-8}$

- An Inversible DWT
- Practical Alternative to Software-based DWT Calculation on AFTAB
- Platform for Future Optimization and Expansions
- Applicable For Different Use Cases

