

# Measurement of the Main Field ( $B_0$ ) Inhomogeneity for the 3T Siemens Magnetom

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EEE474 Foundations of Magnetic Resonance Imaging  
Project Presentation  
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# Introduction

## Off-Resonance Sources [1]

- Main Field Inhomogeneity
- Susceptibility-Induced Field Variations
- Chemical Shift

## How does it affect the imaging?

- Signal Intensity Loss
- Distortions and Blurring
- Curved Slice Profiles [2]



Shading Artifact due to the Main Field Inhomogeneity  
[3]

# Introduction

## How can we quantify the field inhomogeneity?

The phase accumulated by a spin is proportional to the main field:

$$\phi = \gamma ( B_0 + \Delta B ) TE$$

If we acquired 2 scans (at least) with different echo times

$$\Delta \phi = \gamma ( \Delta B ) ( TE_2 - TE_1 )$$

$$\Delta B = \frac{\Delta \phi}{\gamma ( TE_2 - TE_1 )}$$

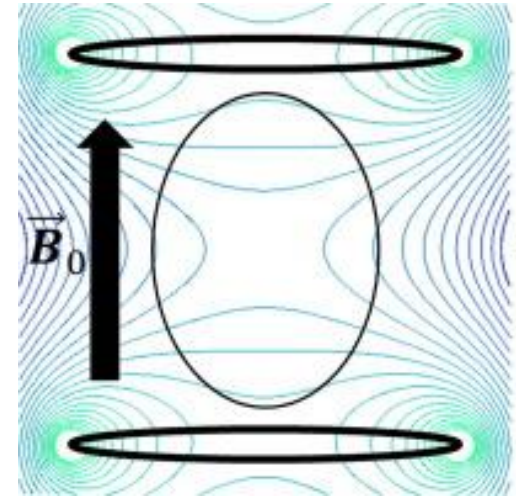
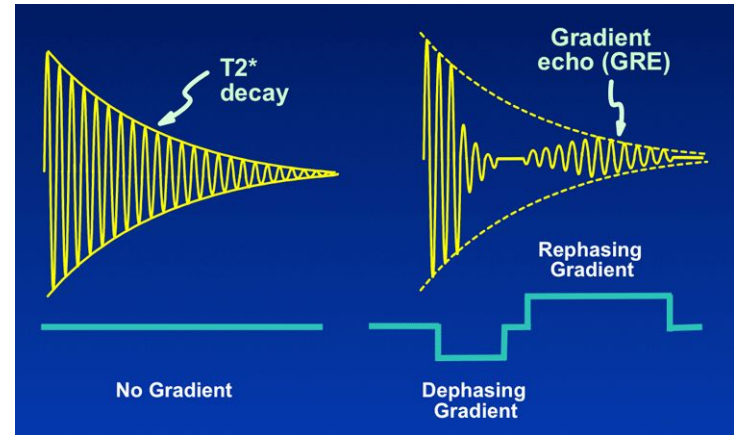


Illustration of  $B_0$

# Methodology: Pulse Sequence Selection

Gradient Echo pulse sequences are more effective for constructing field maps!

- Only one RF pulse is applied :  
Rapid acquisition and reduced scan time.
- Gradient reversal is applied:  
Phase shift due to the field inhomogeneity is detectable [4].



From FID to GRE by Applying Gradient Reversal

# Methodology : GRE Acquisitions and Setup

Separate scans were acquired using a labeled GRE at 3 echo times

TE1 = 5ms

TE2 = 12ms

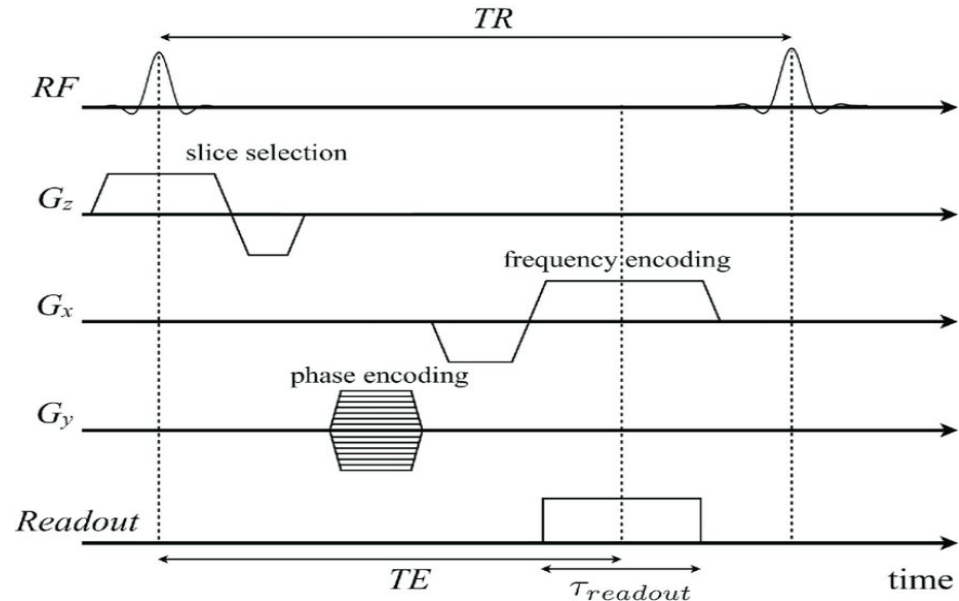
TE3 = 20ms

**Other parameters:**

TR = 100ms

Flip angle = 10 degrees

Resolution = 256x256



Gradient Echo Sequence Timing Diagram

# Methodology: Combining Array Coil Signals

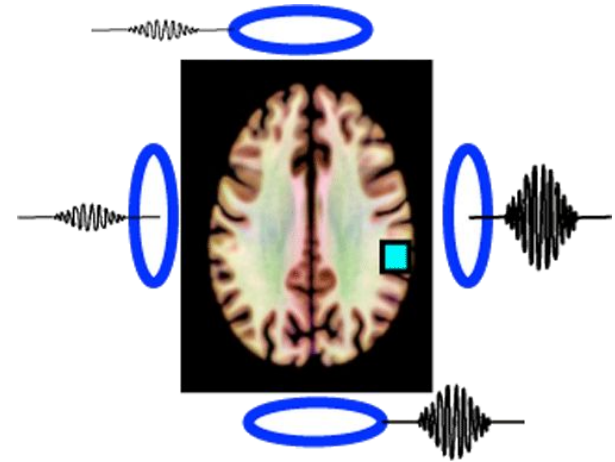
A Siemens 32-channel coil was used to receive the data

→ Increase the signal-to-noise (SNR) ratio [5]

Magnitude images are combined using sum of squares (SoS)

Phase images can be averaged **but** phase is wrapped

→ Solution: work with phase difference between TE's

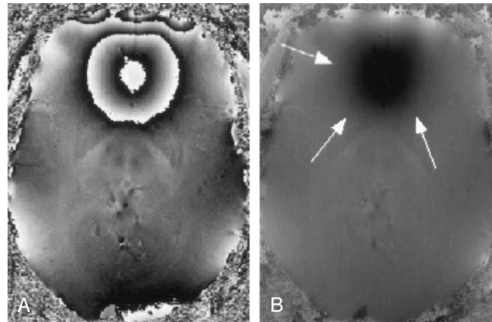


Parallel Imaging Using Multiple Coils

# Methodology: Phase Unwrapping

Matlab built-in function does not support 2D unwrapping

- Fast two-dimensional phase unwrapping algorithm based on sorting by reliability [6]
  - ◆ Robustness : handles phase discontinuities better than traditional methods
  - ◆ Efficient : fast processing ( $\sim 0.5$  seconds) for typical images
  - ◆ Effective: proven through real-world tests to manage noisy data



# Methodology: B0 Field Map Generation

The phase evolution between 2 echos:

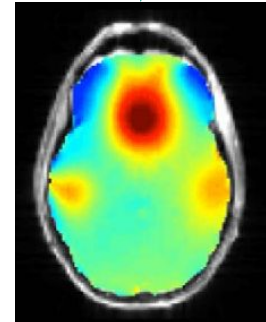
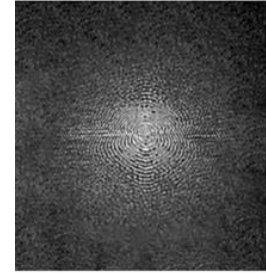
$$\Theta(\vec{r}, n, m) = \angle \left[ \sum_j I_j(\vec{r}, TE_n) I_j(\vec{r}, TE_m) \right]$$

Weighting factor to construct the field map:

$$W(\vec{r}, k) = \frac{M(\vec{r}, k)^2}{M(\vec{r}, k)^2 + M(\vec{r}, 1)^2}$$

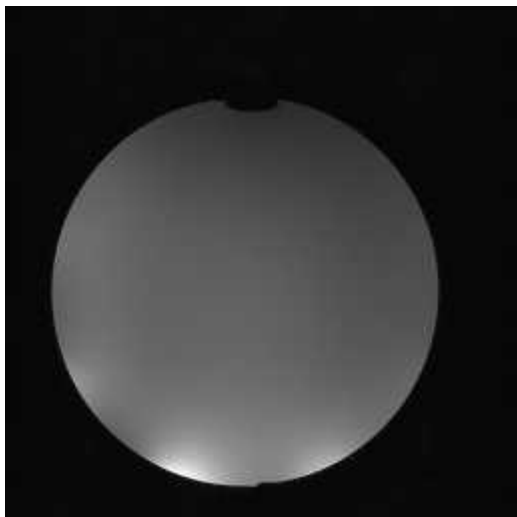
The B0 field map [5]:

$$\Delta B(\vec{r}) = \frac{1}{2\pi\gamma} \frac{\sum_{k=2}^K \Theta(\vec{r}, n, m) (TE_k - TE_1) \cdot W(\vec{r}, k)}{\sum_{k=2}^K (TE_k - TE_1)^2 \cdot W(\vec{r}, k)}$$

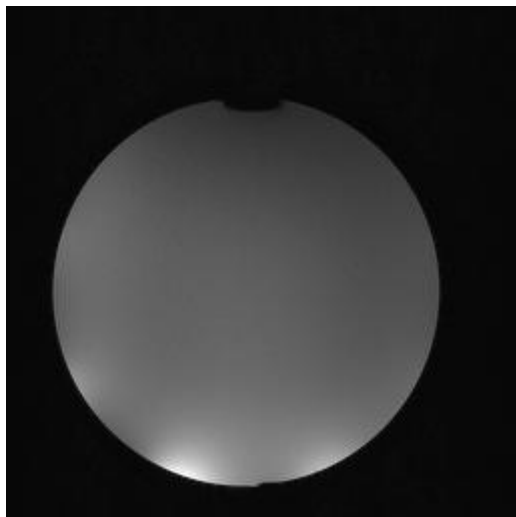




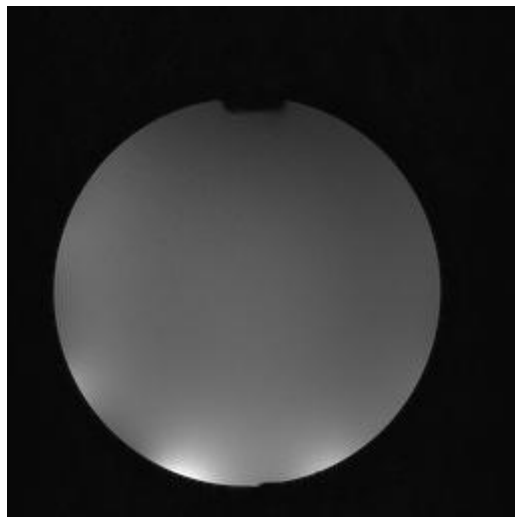
# Results: Magnitude Images



Acquisition with TE1 (5ms)

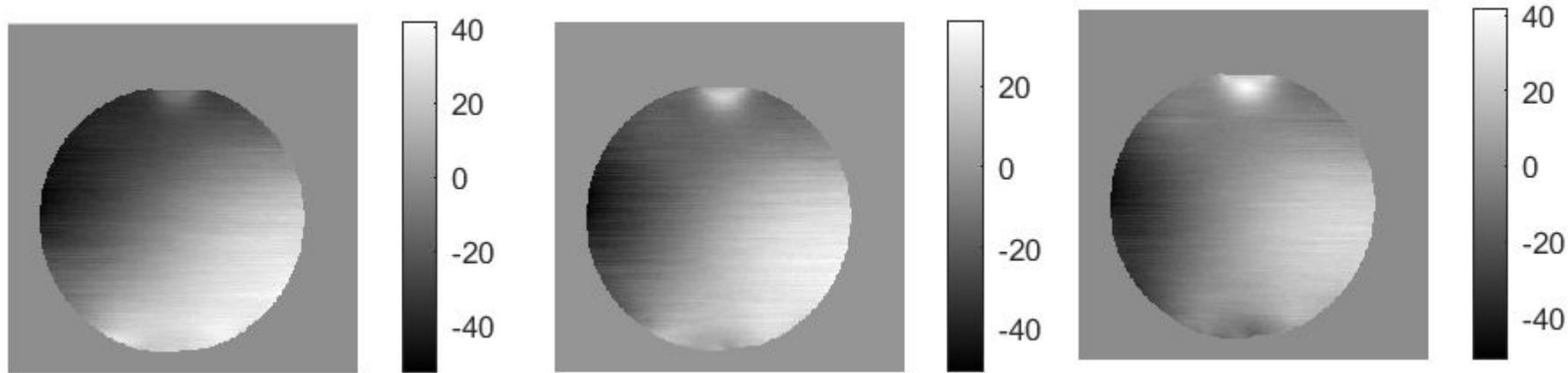


Acquisition with TE2 (12ms)



Acquisition with TE3 (20ms)

# Results: Phase Images

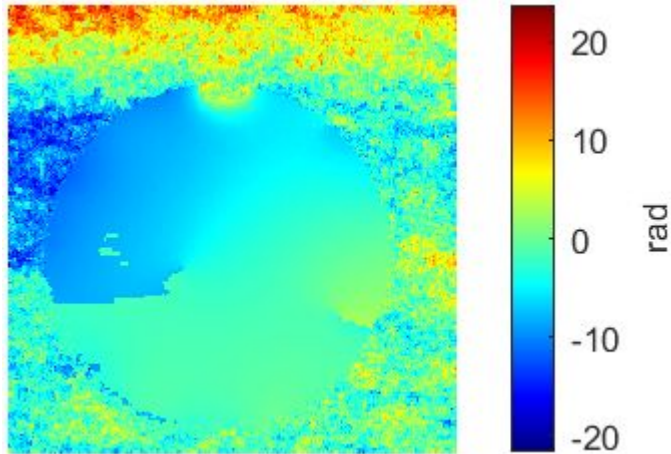


Acquisition with TE1 (5ms)

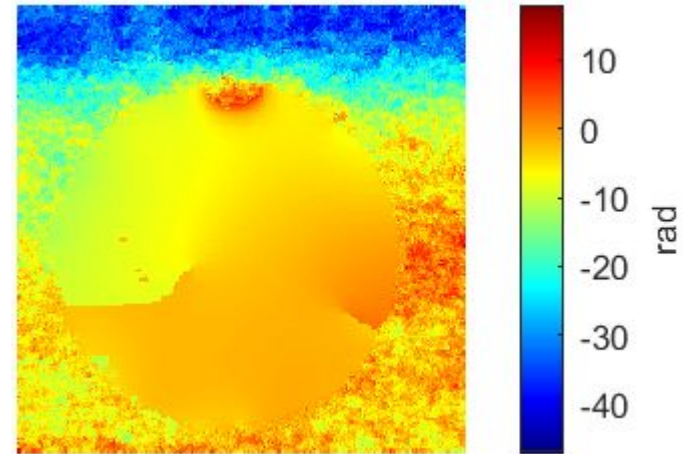
Acquisition with TE2 (12ms)

Acquisition with TE3 (20ms)

# Results: Phase Evolution



Phase Map (TE1, TE2)



Phase Map (TE1, TE3)

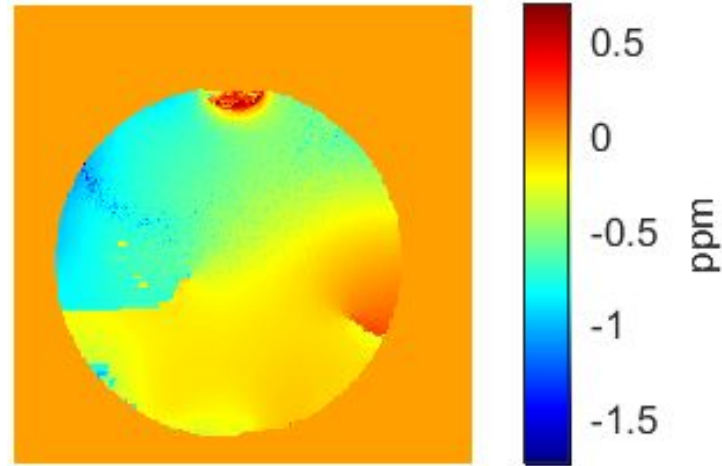
# Results: B0 Field Map



$B_0 = 3\text{T}$

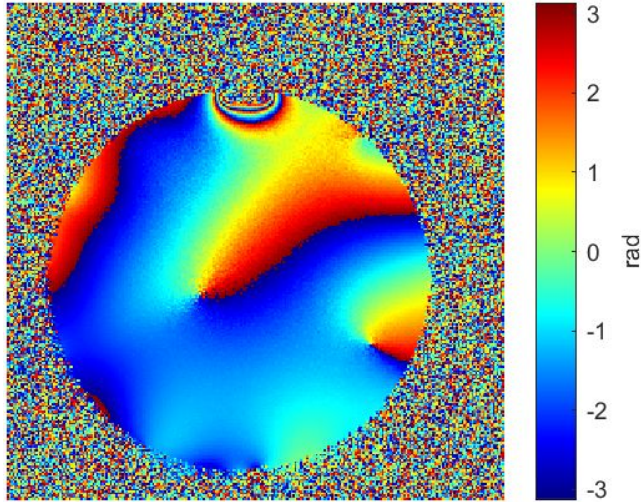
$\Delta B = [-5, 2] \mu\text{T}$

$\Delta B = [-1.5, 0.5] \text{ ppm}$

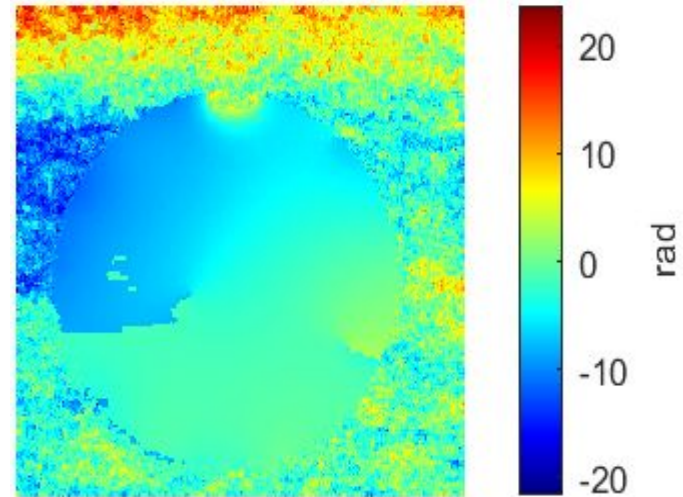


B0 Field Map (Masked)

# Discussion: Wrapped vs. Unwrapped



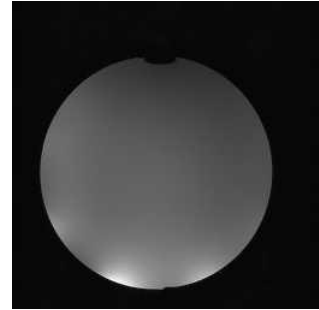
Phase Map (Wrapped)



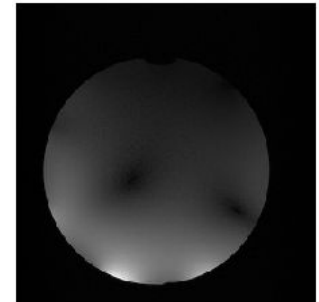
Phase Map (Unwrapped)

# Discussion: Improvements

- Acquiring the phase maps directly from the scanner
- Using the FSL toolbox to unwrap the phase
- Optimized choice of echo times
- Incorporating the coil sensitivity in the reconstruction



Scanner Reconstruction



SoS Reconstruction

# References



- [1] D. G. Nishimura, *Principles of Magnetic Resonance Imaging*, 1.1st ed. Lulu, 2010, pp. 127-128.
- [2] M. W. Haskelon, J.-F. Nielsen, and D. C. Noll, "Off-resonance artifact correction for MRI: A review," *NMR in Biomedicine*, vol. 36, 2023. doi: 10.1002/nbm.4867.
- [3] "Importance of Field Homogeneity," *Questions and Answers in MRI*. [Online] Available: <https://mriquestions.com/why-homogeneity.html>.
- [4] "GRE v SE," *Questions and Answers in MRI*. [Online] Available: <https://www.mriquestions.com/gre-vs-se.html>.
- [5] S. D. Robinson, K. Bredies, et al., "An illustrated comparison of processing methods for MR phase imaging and QSM: combining array coil signals and phase unwrapping," *NMR in Biomedicine*, vol. 30, 2016, doi: <https://doi.org/10.1002/nbm.3601>.
- [6] M. A. Herráez, D. R. Burton, M. J. Lalor, and M. A. Gdeisat, "Fast two-dimensional phase-unwrapping algorithm based on sorting by reliability following a noncontinuous path," *Applied Optics*, vol. 41, no. 35, p. 7437, Dec. 2002, doi: <https://doi.org/10.1364/ao.41.007437>.