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BART



# Think about Motion: Motion = Time

Daniel Mackner

Institute of Biomedical Imaging  
Graz University of Technology

Translational cardiovascular MR Imaging - PhD Training Ulm  
March 18, 2025

# Programme

- MR Image Reconstruction in a Nutshell  
Moritz Blumenthal  
Hands-on: How to use BART
- **Think about Motion: Motion = Time**  
Daniel Mackner  
**Hands-on: Using BART for CMR Reconstruction**
- Real-time MRI  
Philip Schaten  
Hands-on: Real-time reconstruction with BART

# Differences to brain MRI - hurdles in CMR

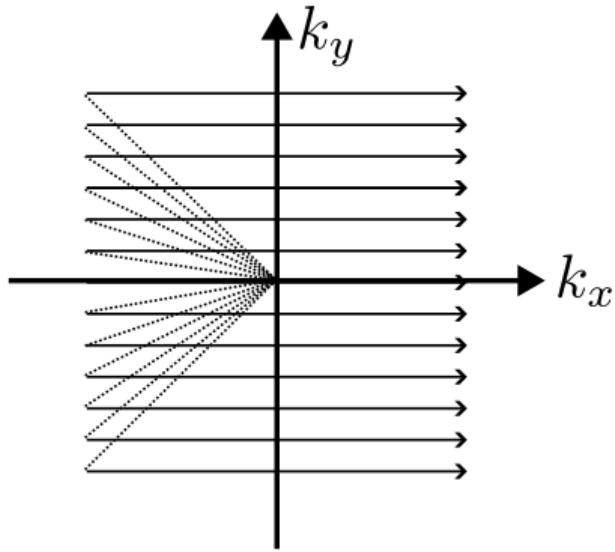
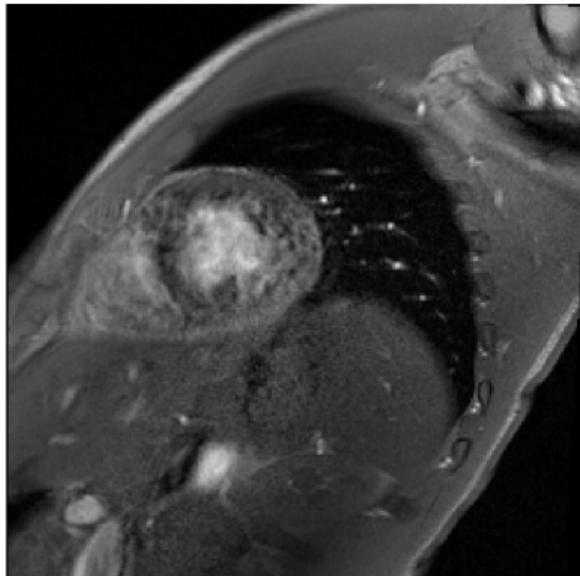
# Outline

- Gating strategies in cardiac MRI
- Why should we use radial sampling?
- What is the advantage of (tiny) Golden Angle?
- How can we reconstruct Non-Cartesian data?
- Temporal regularization?

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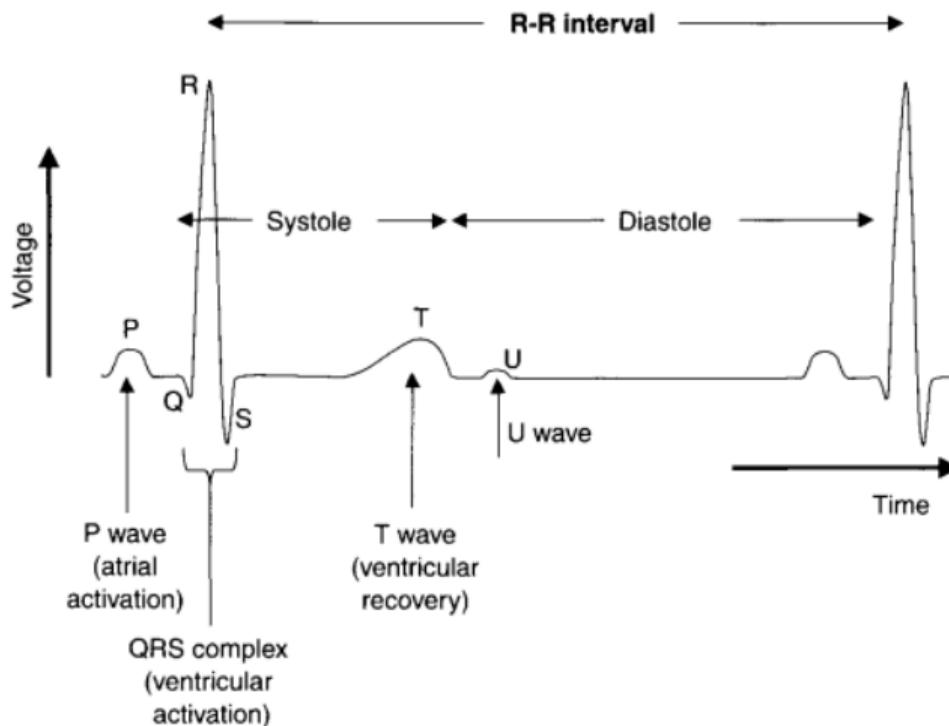
# Naive Cartesian cardiac MRI



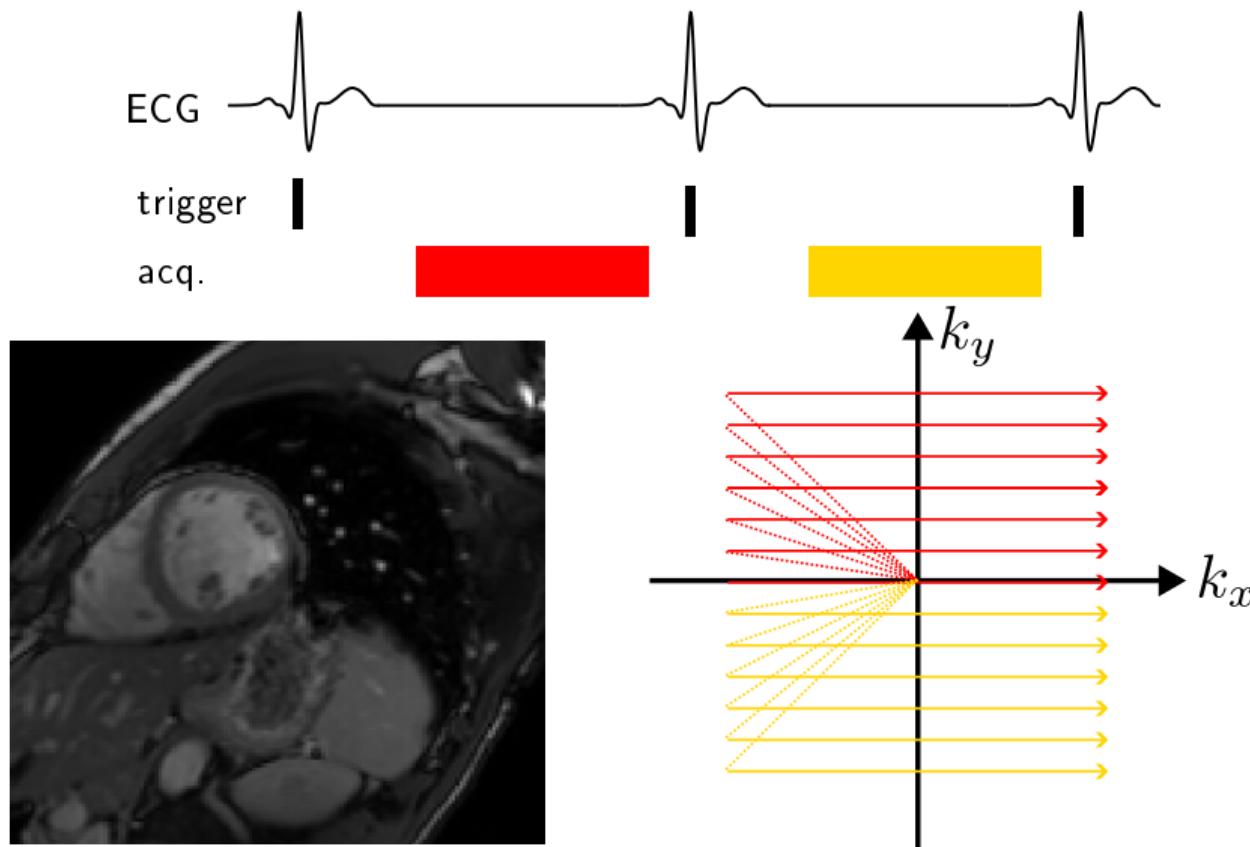
$TR = 5 \text{ ms}$ ,  $BR = 256$ , **TA=1.3 s** (fully-sampled FLASH)

motion artifacts mainly in PE-direction

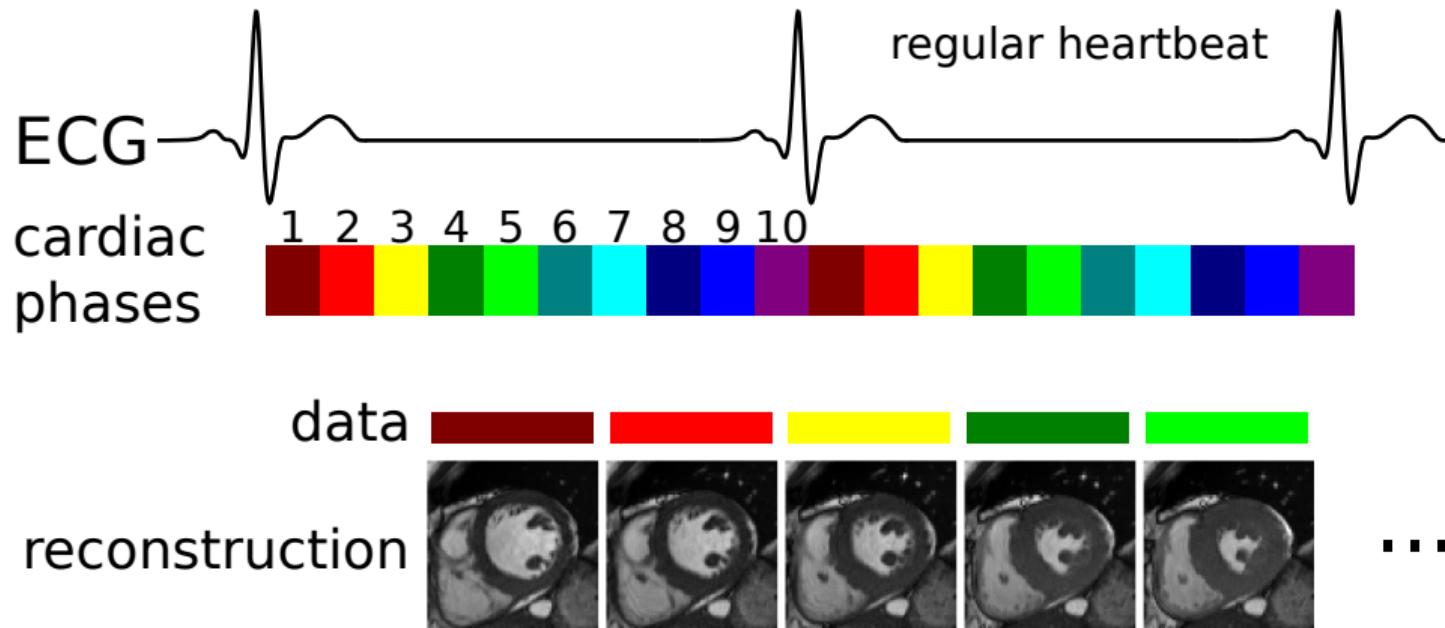
# ECG - basics



# Cartesian cardiac MRI - prospectively triggered



# Cardiac MRI - retrospective gating



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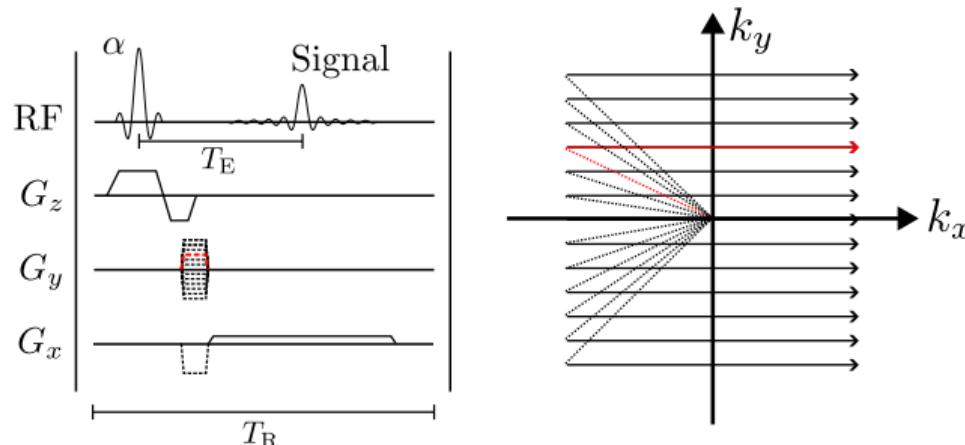
# Sampling strategies

- Signal  $s$  is Fourier transform of the spin density  $\rho$  with k-space trajectory  $k(t)$

$$k(t) = \gamma \int_0^t d\tau G(\tau)$$

$$s(t) = \int_V dx \rho(x) e^{-i2\pi k(t)x}$$

- Cartesian sampling



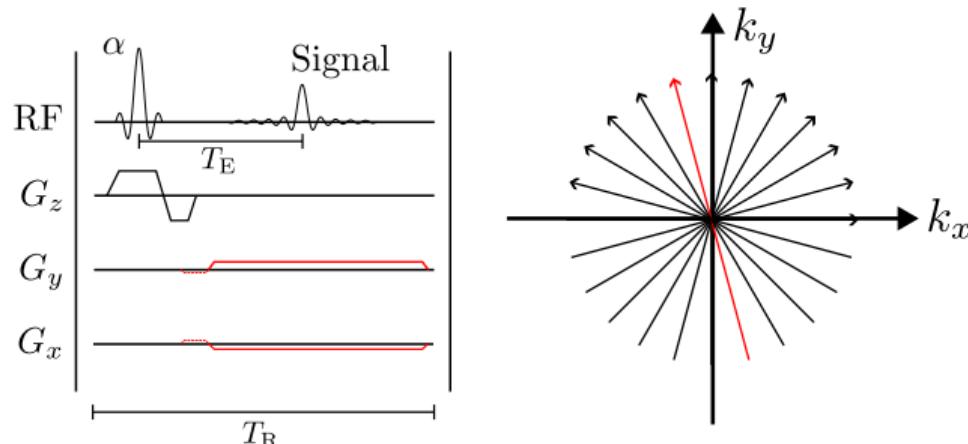
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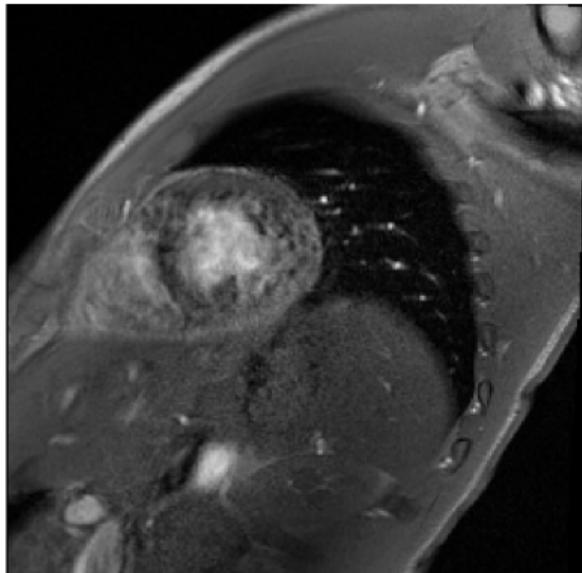
- radial sampling



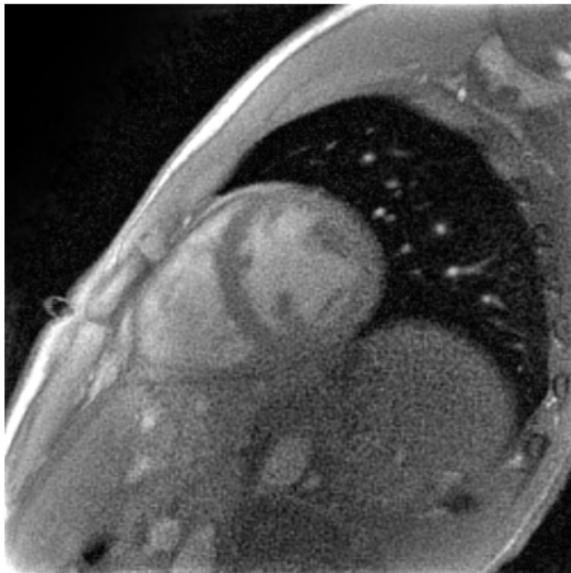
# Why should we use radial sampling?

- motion robust by varying PE and pass of k-space center
  - no ghosting artifacts
- inherent incoherent undersampling property
  - aliasing in Cartesian vs. streakings in radial
- undersampling-induced artifacts look like noise  
(Compressed Sensing)

# Cartesian vs. radial sampling



Cart. FLASH:  $TR = 5 \text{ ms}$ ,  $BR = 256$

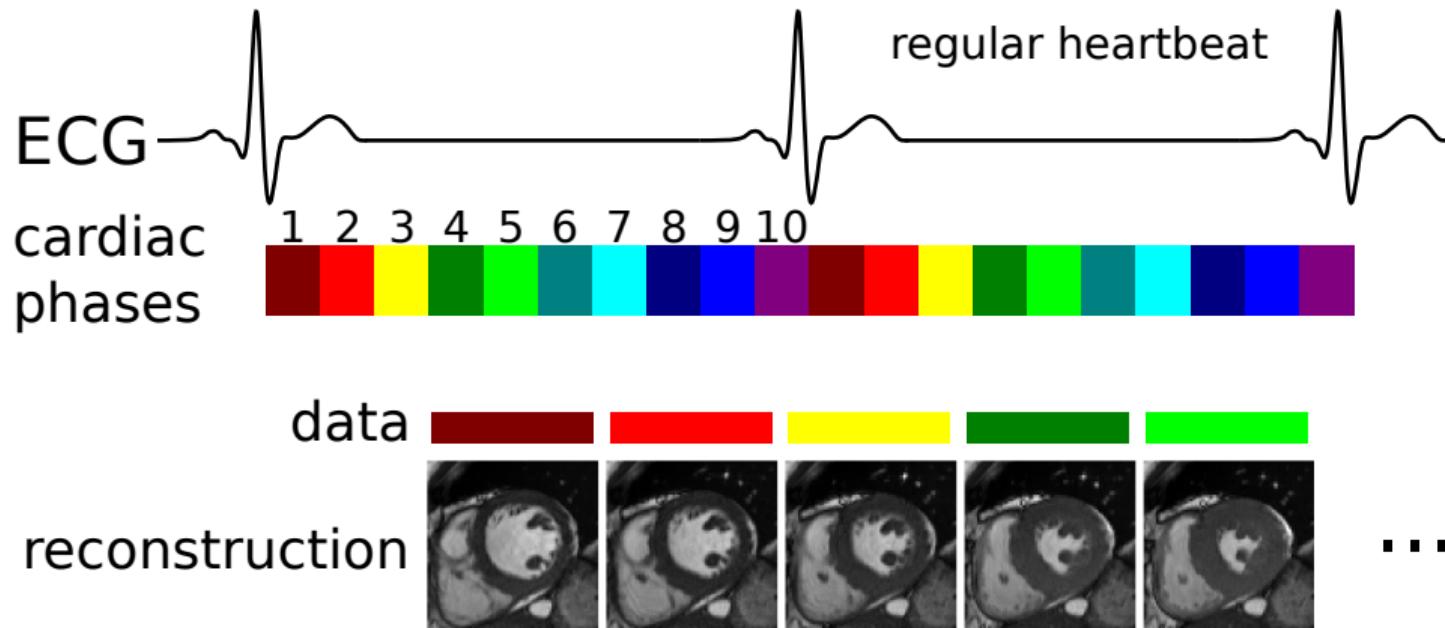


Rad. FLASH:  $TR = 3.5 \text{ ms}$ , 256 spokes

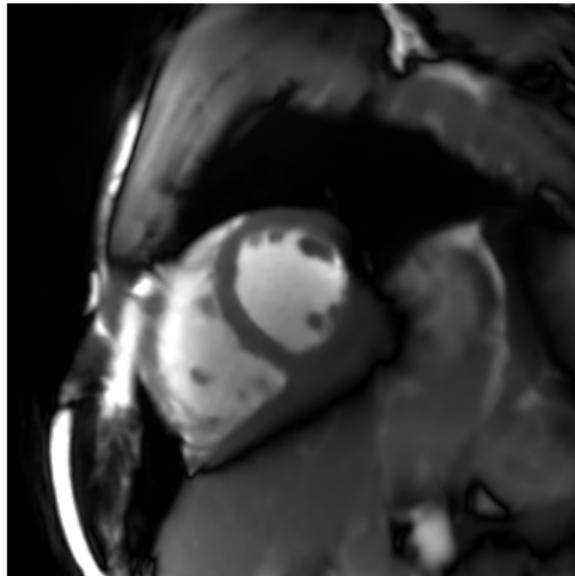
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- What about gating/triggering?

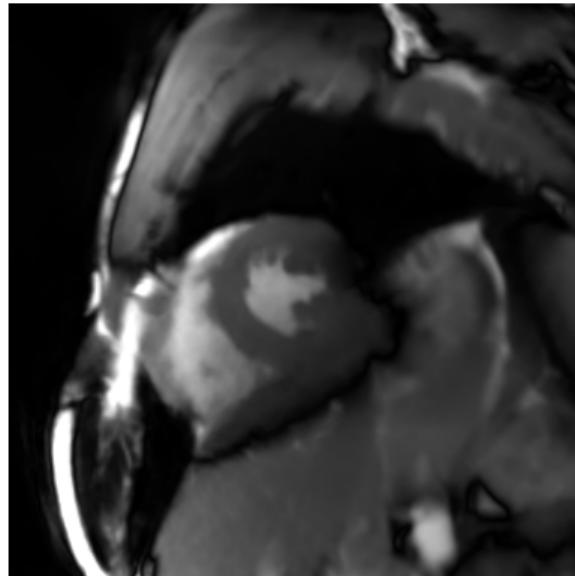
# Cardiac MRI - retrospective gating



# Self-calibration



diastolic phase



systolic phase

- radial lines through the center of k-space
- assumption of mean signal difference originating from the heart
- can eliminate the need to use navigator signals or external device

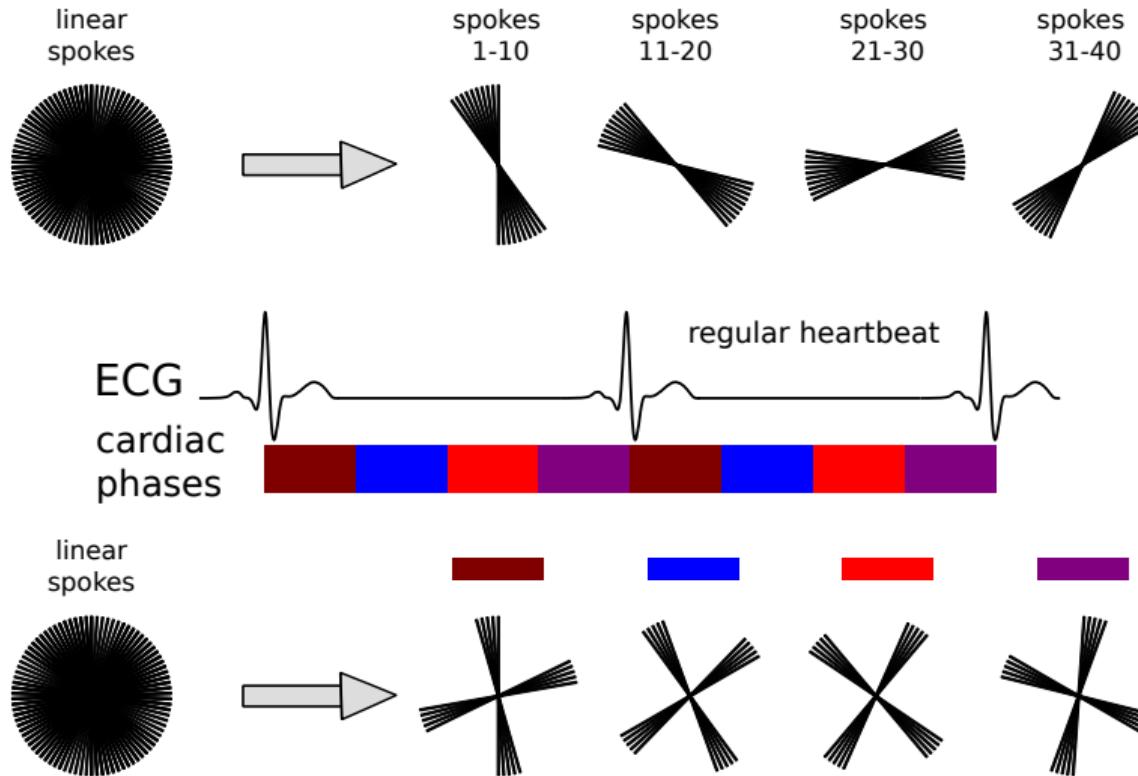
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- What about gating/triggering?
  - retrospective gating by ECG signal
  - self-gating (ECG-free)

# Outline

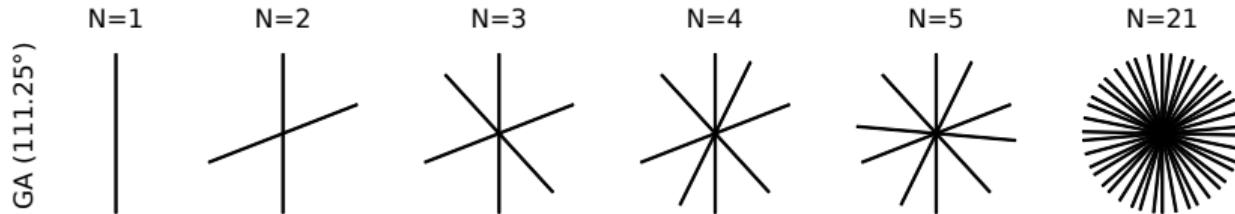
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# What can be the problem with gating in linear ordering?



# What is the Golden Angle?

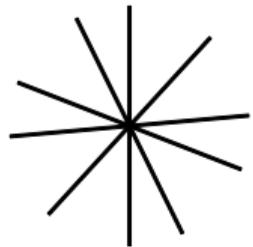
- solve for Golden Ratio (GR)  $\frac{a}{b} = \frac{a+b}{a} \rightarrow GR = \frac{1+\sqrt{5}}{2}$
- for spoke  $n$  we have  $\theta_n = mod\left(\frac{180^\circ}{GR} \cdot n, 360^\circ\right) \approx 111.25^\circ$
- Golden-Angle based radial spokes never repeat each other
- a rather uniform coverage of k-space with high temporal incoherence



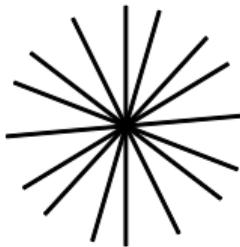
# k-space coverage dependent on number of spokes

- Fibonacci series: 1, 2, 3, 5, 8, 13, 21, ...

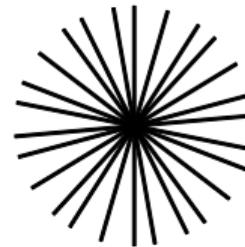
N=5



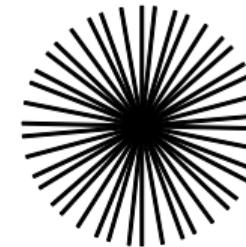
N=8



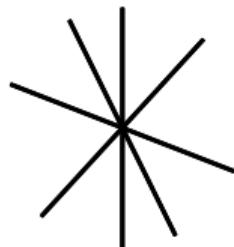
N=13



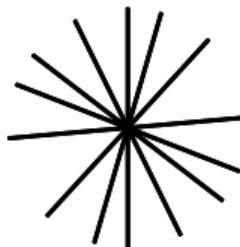
N=21



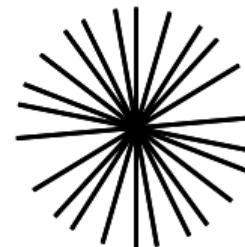
N=4



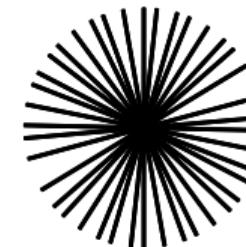
N=7



N=12



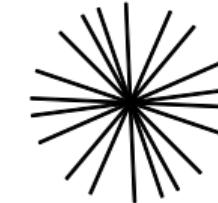
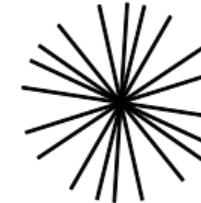
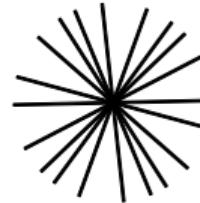
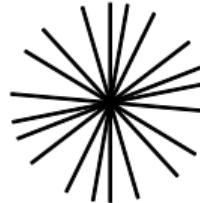
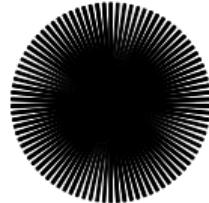
N=20



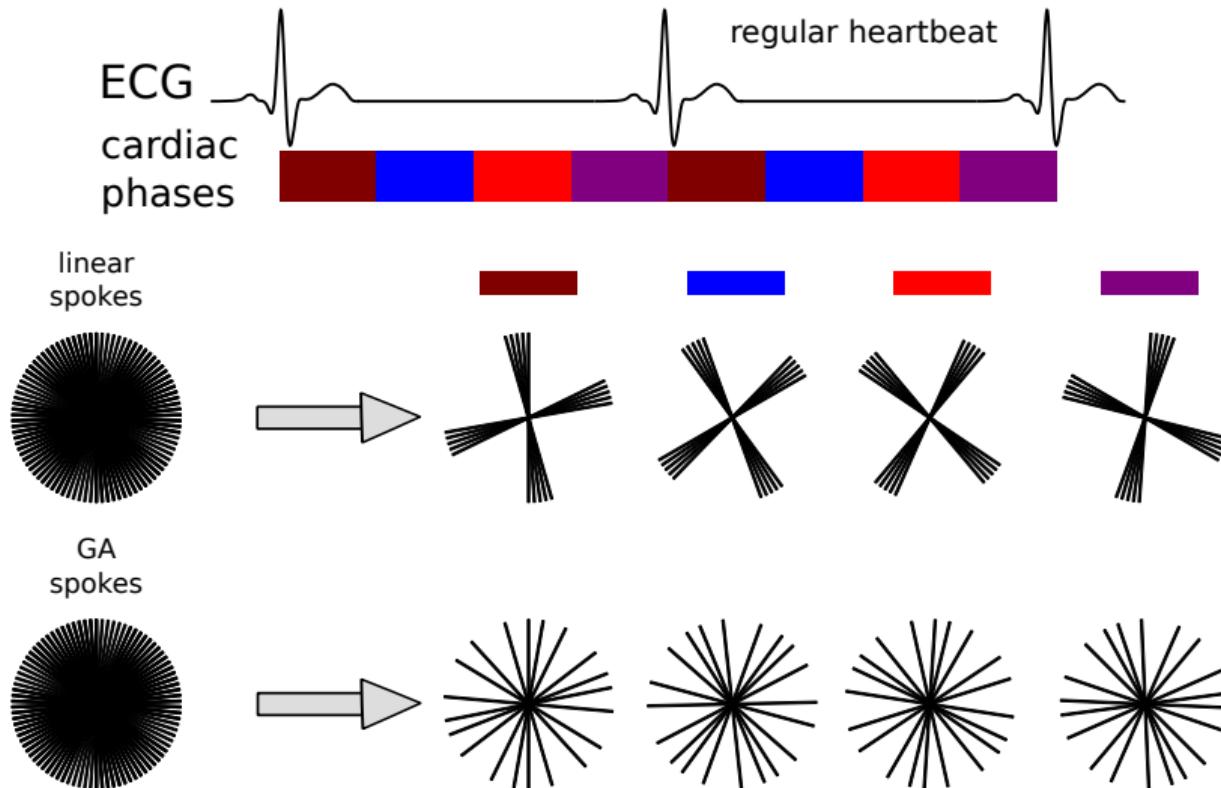
# Linear vs. Golden Angle radial sampling



GA spokes

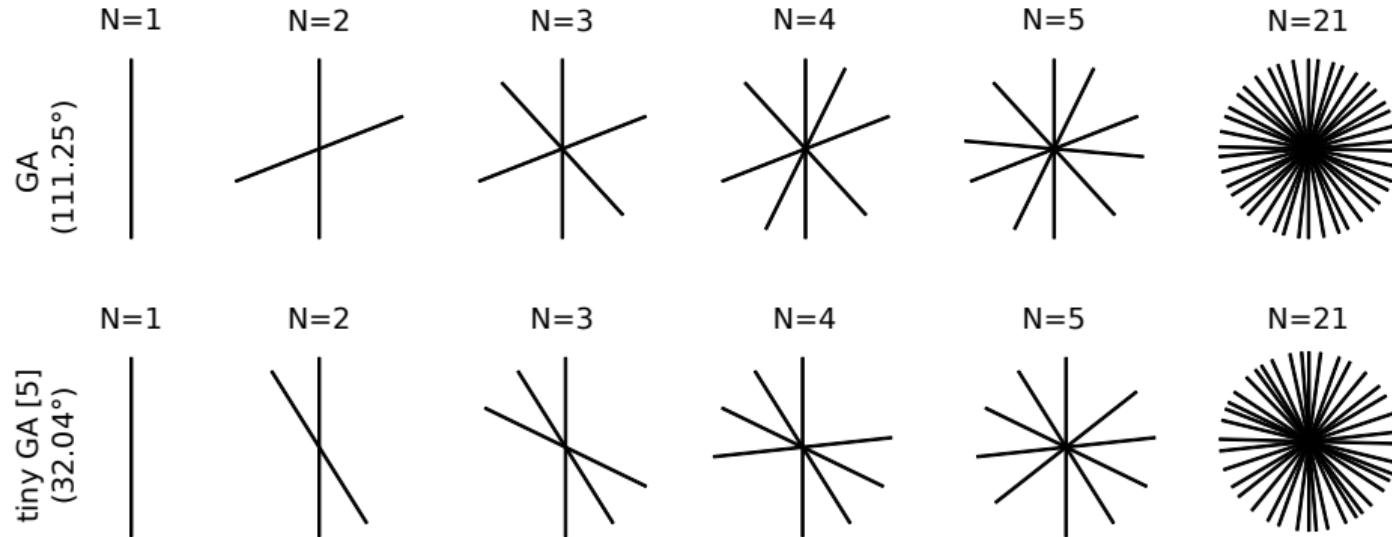


# Linear vs. Golden Angle radial sampling



# What is the tiny Golden Angle?

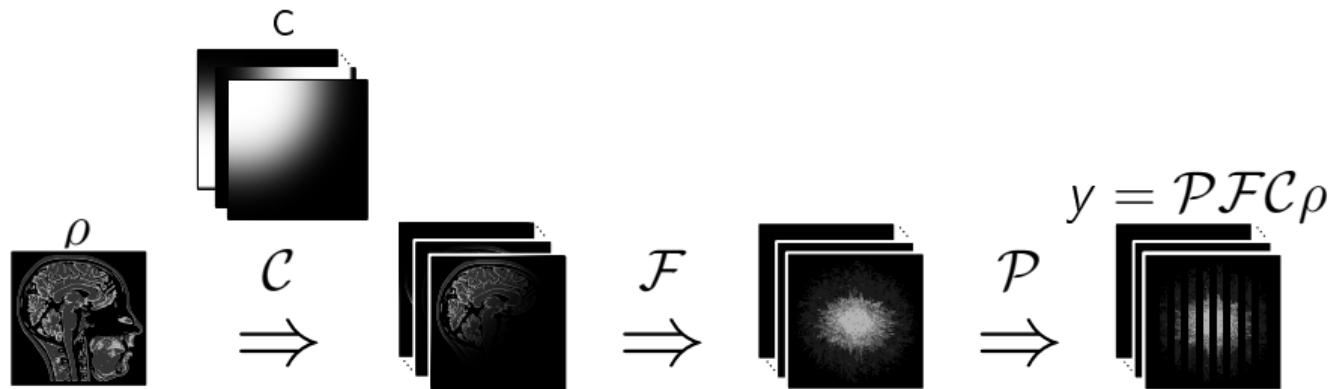
- $\theta_n = \text{mod} \left( \frac{180^\circ}{GR+N-1} \cdot n, 360^\circ \right)$  with  $N > 1$
- reduces sensitivity to eddy currents



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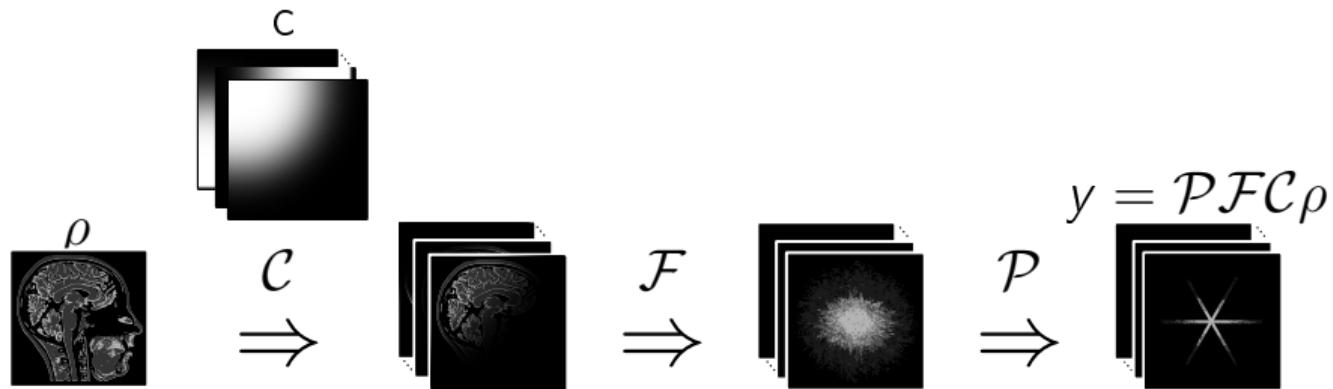
# Forward Model for Non-Cartesian Sampling



The diagram shows the inverse problem formulation. It starts with a target image  $\rho^*$  and a measured image  $y$ . An arrow points from  $\rho^*$  to the measured image, indicating the goal of finding the reconstruction  $\rho^*$  that minimizes the difference between the forward model's prediction and the measured data.

$$\rho^* = \arg \min_{\rho} \underbrace{\|\mathcal{P}\mathcal{F}\mathcal{C}\rho - y\|_2^2}_{A} + \lambda R(\rho)$$

# Forward Model for Non-Cartesian Sampling



The diagram shows the inverse problem formulation. It starts with a reconstructed image  $\rho^*$  (a brain slice) and an operator  $\mathcal{P}\mathcal{F}\mathcal{C}$  (represented by a stack of three square images showing star-like artifacts). These are combined with a regularization term  $R(\rho)$  (represented by a stack of three square images showing a smooth, blurred version of the brain slice) to form the cost function:

$$\rho^* = \arg \min_{\rho} \|\underbrace{\mathcal{P}\mathcal{F}\mathcal{C}\rho}_{A} - y\|_2^2 + \lambda R(\rho)$$

# Non-Cartesian MRI Reconstruction - PICS in BART

$$\rho^* = \arg \min_{\rho} \|\mathcal{P}\mathcal{F}\mathcal{C}\rho - y\|_2^2 + \lambda R(\rho)$$

Cartesian Reconstruction - pattern is provided by mask

```
bart pics -RW:7:0:0.001 -p<pattern> <kspace> <sens> <img>
```

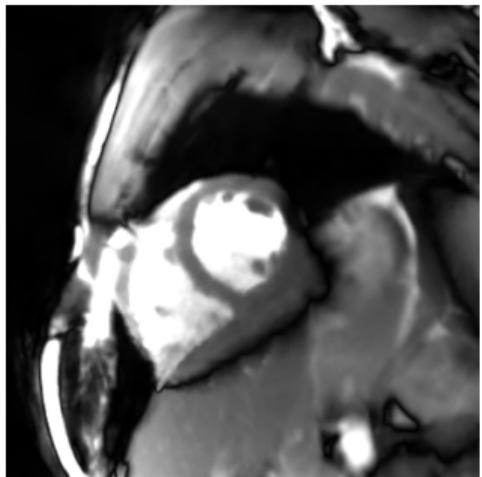
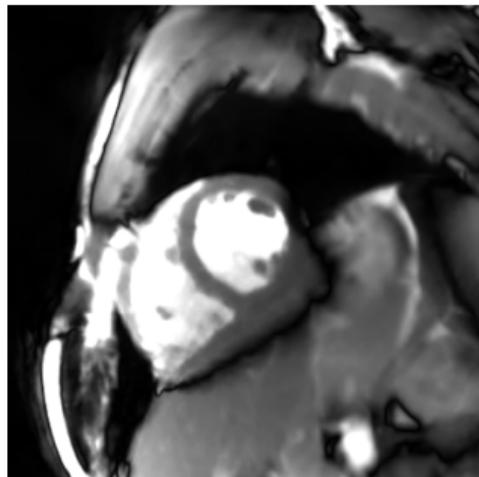
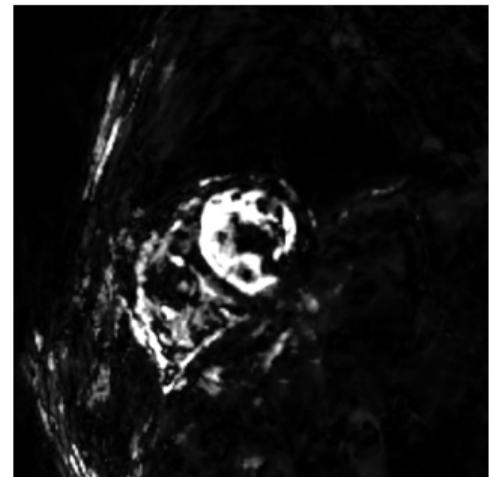
Non-Cartesian Reconstruction - pattern is provided by trajectory

```
bart pics -RW:7:0:0.001 -t<trajectory> <kspace> <sens> <img>
```

# Outline

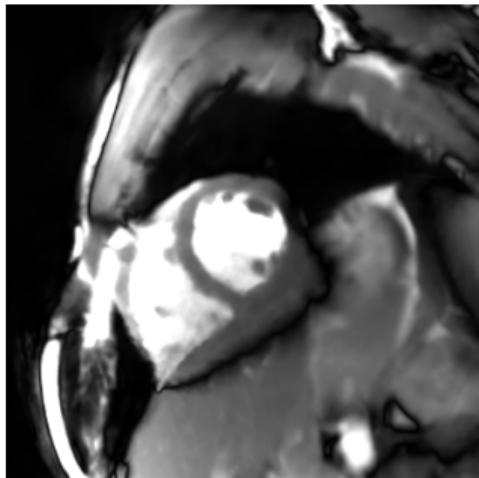
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- **Temporal regularization?**

# Why is temporal regularization useful?

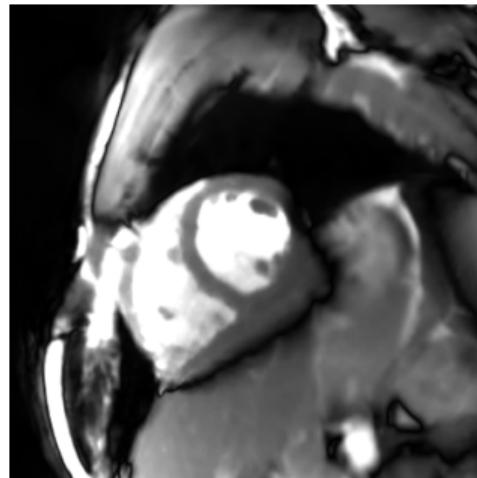
 $\rho_t$  $\rho_{t+1}$  $|\rho_{t+1} - \rho_t| \text{ (scaling } \times 5\text{)}$ 

- How can this sparse difference in time be exploited?

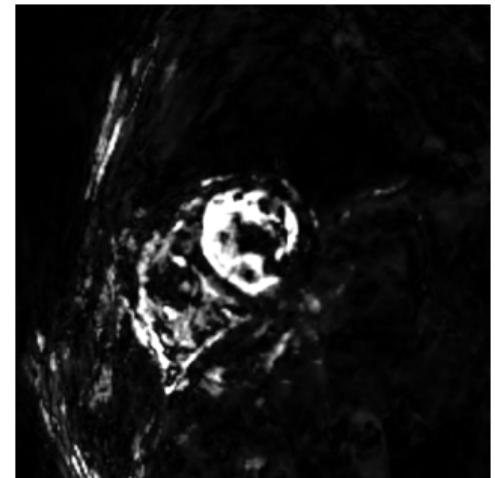
# Why is temporal regularization useful?



$\rho_t$



$\rho_{t+1}$

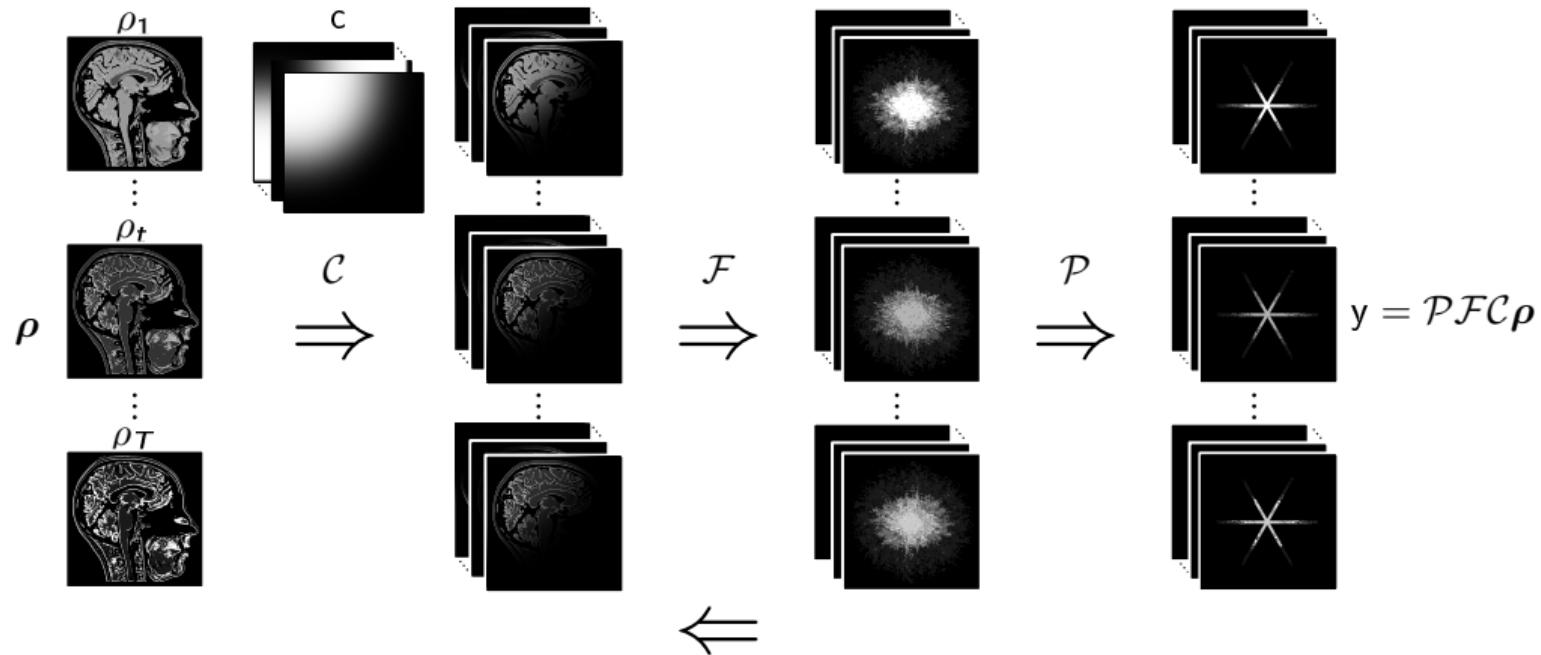


$|\rho_{t+1} - \rho_t|$  (scaling  $\times 5$ )

- How can this sparse difference in time be exploited?
- Additional regularization term in temporal direction

$$R(\rho_t) = \|\rho_{t+1} - \rho_t\|_1$$

# Temporal regularization



$$\rho^* = \arg \min_{\rho} \sum_A \|\underbrace{\mathcal{P} \mathcal{F} \mathcal{C}}_A \rho - y\|_2^2 + \lambda \|W \rho_t\|_1 + \mu \|\rho_t - \rho_{t-1}\|_1$$

# Non-Cartesian MRI Reconstruction with temporal regularization - PICS in BART

$$\rho^* = \arg \min_{\rho} \|\mathcal{P}\mathcal{F}\mathcal{C}\rho - \mathbf{y}\|_2^2 + \lambda R_W(\rho) + \mu R_{TV}(\rho)$$

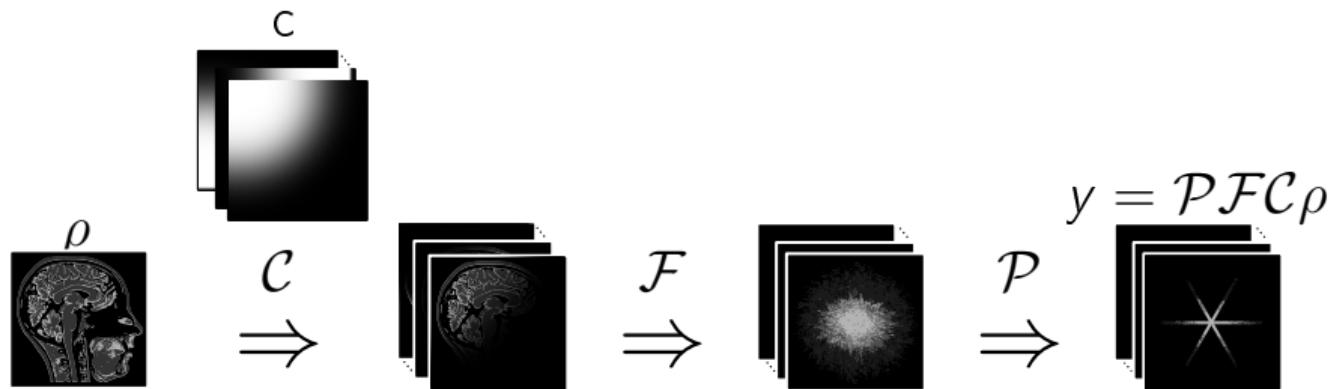
Regularization on spatial position in image

```
bart pics -RW:7:0:0.001 -t<traj> <ksp> <sens> <img>
```

Regularization on spatial position in image and Total variation in time

```
bart pics -RW:7:0:0.001 -RT:1024:0:0.003 -t<traj>  
<ksp> <sens> <img>
```

# MRI Reconstruction as (Nonlinear) Inverse Problem

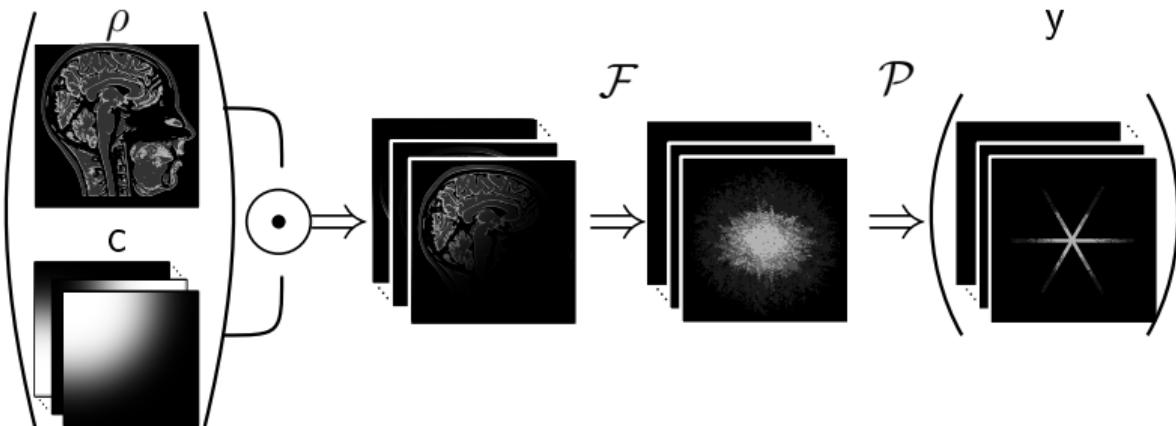


The reconstruction process is modeled as a nonlinear inverse problem:

$$\rho^* = \arg \min_{\rho} \|\underbrace{\mathcal{P}\mathcal{F}\mathcal{C}}_A \rho - y\|_2^2 + \lambda R(\rho)$$

where  $\rho^*$  is the reconstructed image,  $A$  is the operator matrix,  $R(\rho)$  is a regularization term, and  $\lambda$  is the regularization parameter.

# MRI Reconstruction as (Nonlinear) Inverse Problem

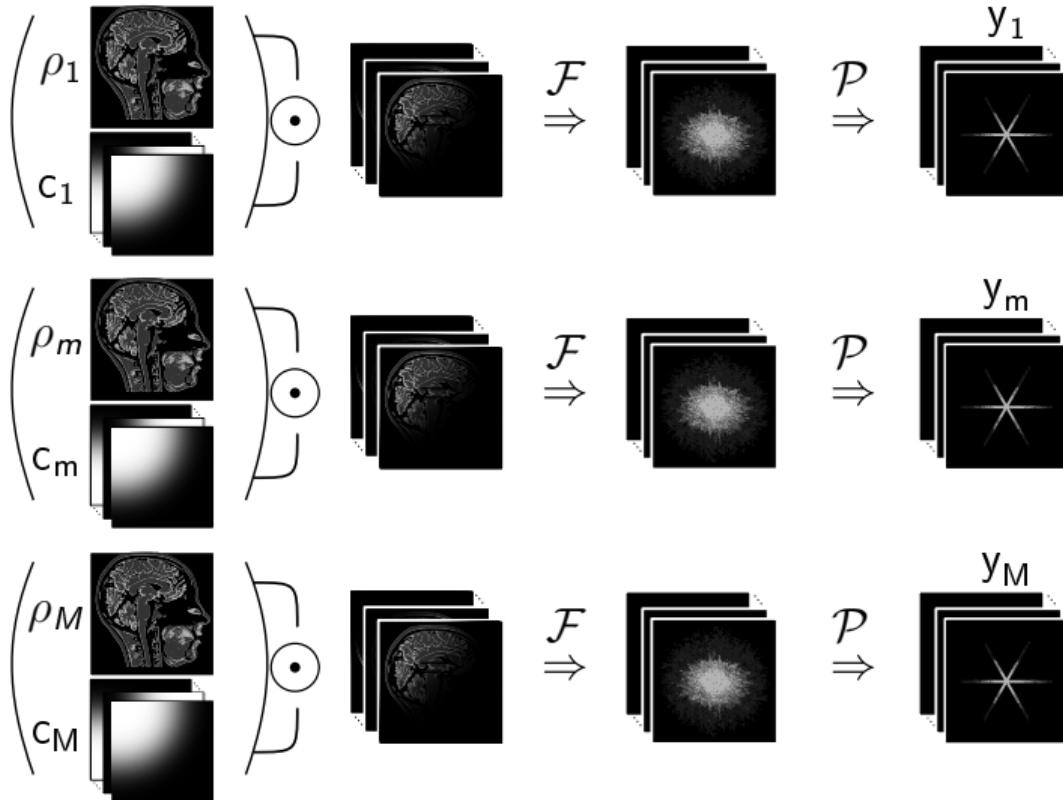


$$F: x = (x_m, c) \mapsto \mathcal{P} \mathcal{F} (c \odot x_m)$$

$$\hat{x} = \underset{x=(x_c, c)}{\operatorname{argmin}} \|F(x) - y\|_2^2 + \alpha \|x_c\|_2^2 + \alpha \|Wc\|_2^2$$

$W$  .. preconditioning matrix (corresponds to Sobolev norm in the original space)

# Coils per motion state





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