

Intracranial hemorrhage localization: A CT imaging pipeline

John Muschelli^{1,*}, Natalie L. Ullman², Elizabeth M. Sweeney³, Ani Eloyan⁴, Daniel F. Hanley⁵, Ciprian M. Crainiceanu⁶

1 John Muschelli Department of Biostatistics, Bloomberg School of Public Health, Johns Hopkins University, Baltimore, MD, USA

2 Natalie L. Ullman Department of Neurology, Division of Brain Injury Outcomes, Johns Hopkins Medical Institutions, Baltimore, MD, USA

3 Elizabeth M. Sweeney, Department of Biostatistics, Bloomberg School of Public Health, Johns Hopkins University, Baltimore, MD, USA

4 Ani Eloyan, Department of Biostatistics, Bloomberg School of Public Health, Johns Hopkins University, Baltimore, MD, USA

5 Daniel F. Hanley Department of Neurology, Division of Brain Injury Outcomes, Johns Hopkins Medical Institutions, Baltimore, MD, USA

6 Ciprian M. Crainiceanu Department of Biostatistics, Bloomberg School of Public Health, Johns Hopkins University, Baltimore, MD, USA

* E-mail: Corresponding jmusche1@jhu.edu

Abstract

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Introduction

Intracranial hemorrhage (ICH) is a neurological condition that results from a blood vessel rupturing into tissues and possibly the ventricles of the brain. Bleeding may cause distension of the brain structures and increase in potentially lethal intracranial pressure (ICP). ICH is a serious condition; it accounts for approximately 10-15% of all strokes, corresponding to an estimated 79,500 annual cases [15] and approximately 30,000 deaths [34] in the US and approximately 5 million cases worldwide [20]. In addition to the increased likelihood of death, ICH has debilitating health effects on survivors who do not have full functional recovery after stroke.

The use of computed tomography (CT) scans allows clinicians and researchers to qualitatively and quantitatively describe the characteristics of a hemorrhage to guide interventions and treatments. CT scanning is widely available and is the most commonly used diagnostic tool in patients with ICH [39]. While much can be understood from careful CT image inspection, detailed quantification of information at the population level is an open problem. Indeed, it is hard, for example, to quantify from visual inspection alone the percent of a particular anatomic ROI engaged by the stroke, compare locations of strokes across patients, and study the association between specific locations and adverse health outcomes.

To address these problems, we will 1) develop an analytic pipeline based on available neuroimaging tools to register patient CT scans to a CT template; 2) create a 3-dimensional (3D) density map of hemorrhages occurring in a population of patients who survived initial ICH and were enrolled in the MISTIE and ICES clinical trials; 3) provide a detailed quantification of hemorrhage engagement of individual neuroanatomic regions within the brain; 4) determine if differences in location relate to two common disability scores: the National Institutes of Health Stroke Scale (NIHSS) [6] and the modified Glasgow Coma Scale (GCS) [46, 45]; and 5) generate a stroke region of engagement that is likely to be associated with adverse health effects and test its predictive performance using within-sample validation.

It is a matter of debate whether the location of the ICH is relevant to functional outcome in patients who survived to make it to the hospital [7]. For example, Hemphill et al. [17] found that infratentorial

ICH location, intraventricular involvement, and ICH volume, which may represent a number of anatomic locations, all predict 30-day mortality. Conversely, Chuang et al. [9], and Diringer, Edwards, and Zazulia [12] found that the site of ICH **univariately** was associated with 30-day mortality, but was not statistically associated after adjusting for other covariates. Following the result that hydrocephalus was an independent predictor of 30-day mortality [12], Phan et al. [30] found that hydrocephalus was an independent prognostic indicator only for the group with hemorrhages in the putamen and not for those with hemorrhages in the caudate  thalamus. In contrast, other studies have not observed location of the ICH predicting prognosis [31, 40, 11, 5, 22, 23, 33, 36, 16, 8].

Other trials have estimated the effects of surgery in a sub-population of ICH patients on health outcomes. Phase I of the Surgical Trial in Intracerebral Haemorrhage (STICH I) found treatment effects of hemorrhage reduction through early surgery in a subset of patients who had bleeds in the proximity of the brain lobes (1 cm from the cortical surface of the brain) [24]. However, when the effect was re-examined in the second phase of the trial (STICH II), which included only patients with superficial lobar hematomas, the treatment effect was not found to be statistically significant [25]. Although STICH II did not identify a statistically significant treatment effect, this may be due to sub-optimal definition of localization. In the “Guidelines for the Management of Spontaneous Intracerebral Hemorrhage” Morgenstern et al. [26] noted that: “other randomized trials have had too few patients to determine outcomes in subgroups by location, randomized only patients with deep ICH, or did not report these results”. Moreover, the localization of ICH and its evolution before and after treatment administration may actually be a crucial baseline or longitudinal characteristic of the stroke that could predict whether treatments are effective, may be a confounding factor of treatment and outcomes, and may relate to ICH recurrence [13].

However, even the coarse classification of hemorrhage location is complicated, which may lead to labeling confusion even among the best trained neuroimage scientists. Indeed, a hemorrhage may extend into multiple brain areas, may affect different tissue classes, and may break through the ventricular wall causing the hemorrhage to spread to other areas of the brain. Such problems would challenge even the best scientists, as it becomes time-onerous to do anything more than calling a single region as the primary affected anatomic region (e.g. caudate or putamen) or describing the edge of a hemorrhage by an average or minimum distance to a given landmark [49]. Also, increased long- or short-term disability that corresponds to a significant difference in hemorrhage volume may be modulated by hemorrhage location. Alternatively, hemorrhage increases after a stabilization period may result in no changes in functional indices depending on the brain regions involved. Hence, there is a need for detailed information of brain hemorrhage location and its association with the stroke severity, while controlling for ICH volume. Such detailed localization information can be obtained by registering scans to a common template and by using the detailed anatomical information in the template to provide refined anatomical localization information.

Previous CT neuroimaging studies have not used registration-to-template-based methods for detailed location quantification, most likely due to a lack of a CT template brain. Registration to template space is a crucial first step for the type of analysis we are describing here, as all patient scans are located in the same stereotaxic space **and can be** information may be combined across scans. Recently, Rorden et al. [38] published the first CT template of healthy adults in its MNI (Montreal Neurological Institute) space representation. Along with this template, Rorden et al. [38] released software for CT image registration to the template. This software provides an important analytic step forward **over the** previous available **tools**. Indeed, previous studies have used average CT images as a template, but the patient population consisted of people affected by a specific neurological condition (**crebrovascular infarcts**) and were not in MNI space [19]. In addition, many other studies have co- registered CT images to concurrent (or temporally proximal) MRI images from the same patient [14, 10, 4, 29]. This registration process is **very** useful when structural MRIs are concurrently acquired with CT images. In the clinical trials we investigate here the CT images have always been acquired according to the trial protocol, whereas MRI sequences were only acquired according to the local practices, which varied quite a bit by modality and

frequency. Therefore, we require a CT-only pipeline. Other methods have used CT image registration directly to an MRI template, but using a CT template provides a simpler registration as the reference image and template image are the same modality [43, 21, 32].

Most importantly, this type of detailed mapping of strokes has never been done in the context of the highly visible MISTIE and ICES stroke clinical trials. MISTIE is the Minimally Invasive Surgery plus recombinant-tissue plasminogen activator (rtPA) for Intracerebral Evacuation trial and ICES is the Intraoperative CT-Guided Endoscopic Surgery for ICH trial. MISTIE was a phase II clinical trial with the goal of determining the safety, efficacy, and long-term effects of treatment of ICH using thrombolytics. ICES was a simultaneous phase I trial with the same inclusion/exclusion criteria as MISTIE and the goal to determine the effect of endoscopic surgery as opposed to thrombolytic therapy for hematoma removal. No treatment effects are of interest in our analysis and any scan, demographic, or functional measure was taken prior to randomization.

Materials and Methods

All statistical analysis was done in the R statistical programming language (<http://cran.r-project.org/>). We used the `oro.nifti` package [47] for reading and visualizing brain images and the `ggplot2` package [48] to visualize histograms.

Subjects and Demographics

The study consists of 111 patients from MISTIE ($N = 94$) and ICES ($N = 17$) recruited from 26 centers. Patients were eligible if: he/she were aged 18 to 80 years old with a spontaneous ICH of greater than 20cc that did not require an extraventricular drain (EVD), were non-pregnant, had a historical Rankin Scale [35, 44] score of 1 and a diagnosis that excluded other conditions such as ruptured aneurysms, arteriovenous malformations, or other neurovascular anomaly (for full criteria, see Mould et al. [27]). CT and clinical data were previously collected as part of the Johns Hopkins Medicine IRB-approved ICES and MISTIE research studies with written consent provided by participants. Each site adhered to local ethical procedures and consented in participation of the study. All clinical data was deidentified by using a unique patient identifier and CT images were anonymized to remove any patient identifying information.

The NIHSS and GCS scores were recorded at enrollment into the study; 3 patients did not have a recorded NIHSS score, 1 patient did not have a recorded GCS score, and these patients were excluded from the analyses associating NIHSS and GCS scores and location, respectively. All patients were included in the construction of the 3D histogram image. Histograms of NIHSS score, GCS score, age, and baseline ICH volume are shown in Figure 1, and the descriptive statistics of age, sex, NIHSS and GCS scores are shown in Table 1. These measures reflect different aspects of a patient's health: the NIHSS score reflects a stroke impact, the GCS score reflects a patient's level of consciousness. The NIHSS scores indicate large heterogeneity of disease burden, with a range between 2 (no stroke symptoms) to 41 (severe stroke). This heterogeneity is similarly reflected in the GCS score distribution with a range of 3 (deep unconsciousness) to 15 (fully awake person). The age of the patients is between 33 and 80 years, with a mean of 60.8 years. Women comprise 31.5% of the dataset.

[Figure 1 here.]

[Table 1 here.]

Imaging Data

CT images were acquired for all patients, with site-specific scanning parameters. Scans were acquired using GE ($N = 46$), Siemens ($N = 37$), Philips ($N = 20$), and Toshiba ($N = 8$) scanners. Gantry

tilt was observed in 87 scans. Slice thickness of the image varied within the scan reconstruction for 14 scans, which we will refer to as variable slice thickness. For example, if a scan was reconstructed with 10 millimeter (mm) slices at the top and bottom of the brain, which are not of interest, but with 5mm slices in the middle where the hematoma is seen (see Figure 3a). Therefore, the scans analyzed had different voxel dimensions and image resolution prior to registration to the template. Different reconstructions of CT images are not available via the data-acquiring center, and represent how scans are presented for evaluation in many diagnostic cases.

Hemorrhage Segmentation and Location Identification

To register the CT scan to the CT template, the hemorrhage was excluded from the algorithm, i.e. “masked out”, using manual ICH segmentations. ICH was ~~designated~~ on CT scans using the OsiriX imaging software by expert readers (OsiriX v. 4.1, Pixmeo; Geneva, Switzerland). ~~These~~ readers employed a semiautomated threshold-based approach using a Hounsfield unit (HU) range of 40 to 80 to select potential regions of ICH [3, 41]. Binary image masks were created for the hemorrhage region of interest (ROI) by setting ~~pixel intensities~~ to 1 if classified as hemorrhage, and 0 otherwise. ~~These~~ readers ~~classified~~ the region most engaged by the ICH ~~previous to this analysis as a standard hemorrhage characteristic~~.

Image Processing: Brain Extraction, Reorientation, Registration

CT brain images and the binary mask were exported from OsiriX ~~in~~ DICOM (Digital Imaging and Communications in Medicine) format. Images with gantry tilt were corrected using a customized MATLAB (The Mathworks, Natick, Massachusetts, USA) user-written script (<http://bit.ly/1ltIM8c>). Images were converted to the Neuroimaging Informatics Technology Initiative (NIfTI) data format ~~by~~ dcm2nii (2009 version, provided with MRIcro [37]). Images were constrained to values –1024 and 3071 HU to remove potential image rescaling errors and artifacts. No interpolation was done for images with a variable slice thickness. Thickness was determined from the first slice converted and was assumed homogeneous throughout.

Brains were extracted to remove skull, eyes, facial and nasal features, extracranial skin, and more importantly non-human elements of the image captured by the CT scanner, such as the gantry, pillows, or medical devices. Using a variant of a previously published brain extraction protocol [38], removal of ~~aforementioned~~ elements ~~were~~ performed using the brain extraction tool (BET) [42], a function of the FSL [18] neuroimaging software (v5.0.4). Images were thresholded to a brain tissue range (0–100 HU) and BET was applied, using a fractional intensity threshold of 0.01. An image with its brain-extracted counterpart can be seen in Figure 2.

In order to use statistical parametric mapping (version 8, SPM8, Wellcome Trust Centre for Neuroimaging, London, United Kingdom) spatial registration algorithm, images must be centered at the line between anterior commissure (AC) and posterior commissure (PC). This AC-PC line was automatically estimated from ~~this~~ brain-extracted image using a custom MATLAB script (<http://bit.ly/1gUqMDw>), ~~yielding a~~ transformation matrix. The non-brain-extracted image and binary mask were re-centered using this transformation matrix, ~~which is required for the~~. The binary hemorrhage mask was smoothed using a Gaussian smoother with a full width at half maximum (FWHM) of 3mm. The brain image was masked by the inverse of the smoothed hemorrhage mask before registration.

The image was then spatially registered to the CT template using the Clinical toolbox [38], which employs SPM8’s unified normalization-segmentation routine [2] in MATLAB. The smoothed hemorrhage mask was transformed into the template space using the estimated registration transformation. The registered smoothed hemorrhage mask was then thresholded using the following rule:

$$\text{Icon} \quad v_{ij} \frac{\min(I_i) + \max(I_i)}{2}$$

where v_{ij} denotes voxel j for smoothed mask for person i , denoted I_i . This corresponds to voxels in the template space being classified as ICH if the transformed voxel on the transformed smoothed mask was larger than the midrange of the transformed smoothed mask.

Assessing Registration

Determining the quality of registration was done qualitatively by visual inspection. We acknowledge that visual inspection is subjective but there is no gold standard for assessing registration results and analysis of registration quality is not commonly done with large deformations of tissue as in patients with ICH.

No scans were excluded due to inadequate registration.

Histograms of ICH in the Brain

To visualize and describe the localization of lesions, we first combined information from registered masks of 111 patients. Using the registered ICH masks we obtained the 3-dimensional (3D) histogram of the ICH localization for our study population. More precisely, for every voxel location in the template space, we calculated the proportion of patients who have an ICH at that particular voxel. As we can only present the results as pre-selected slices of the 3D volume, we used the R package `brainR` to create an 3D interactive map of the 3D histogram. The interactive map is located at http://muschelli2.github.io/CT_Pipeline/index.html.

Prediction of Functional Score Based on Hemorrhage Location

~~Although summaries of the population level ICH engagement is useful, one area of interest is finding the relationship between ICH location and functional score. We evaluated the association between hemorrhage location and stroke severity as measured by the total NIHSS score or GCS score by a series of models. In the population, patients had an ICH at a total of 1045174 voxels. We limited our analysis of each functional score to voxels in the template space where more than 10 patients exhibit lesions for identifiability of the models and to prevent voxel level effects resulting from only few patients having ICH at those locations. This threshold included 166202 voxels in our analysis. At each of these voxels, we ran a linear regression model:~~

$$Y_i = \beta_0 + \beta_1(v) ICH_i(v) + X_i^t \gamma + \epsilon_{iv}, \quad (1)$$

where Y_i was either the total NIHSS score or GCS score for patient $i = 1, \dots, 111$, $ICH_i(v)$ is a binary indicator where $ICH_i(v) = 1$ if patient i 's ICH mask has a 1 at voxel v of the template space and $ICH_i(v) = 0$ otherwise, X_i^t is a vector of patient-specific confounders with effects and ϵ_{iv} are treated as independent homoscedastic errors. The vector of confounders, X_i , either was excluded for “unadjusted” voxel-level models, or contains a combination of 3 patient-specific confounders, age, sex, and total baseline ICH volume (TICHVol) in an adjusted model. We also ran a simple unadjusted Wilcoxon rank-sum test on Y at every voxel to see if a non-parametric rank-based test resulted in a different relationship between ICH location and functional score.

P-values of each voxel-wise regression model of the functional scores on ICH presence were calculated, corresponding to the hypothesis test $H_{0,v} : \beta_1(v) = 0$, or in the case of the Wilcoxon rank-sum test: $H_{0,v} : Score(ICH(v) = 1) = Score(ICH(v) = 0)$, where $Score$ denotes the distribution of functional scores of patients that either did or did not have ICH at the given voxel v . The p-value images displayed were not corrected as the goal is to see potential “hot spots” of ICH that relate to functional outcome.

We corrected the p-values, within each analysis of functional scores, using a Bonferroni correction with $\alpha = 0.05$. Some of the voxels were identical for presence for ICH over the population, e.g. voxels 1 and 2 each had the same people having ICH and same people not having ICH at that location. We excluded these from the correction, using only then number of unique tests ($N = 48775$).



Region of Interest Generation and Analysis

In order to create a potential patient-level covariate which summarize ICH location information, we created potential regions of interest (ROIs) by selecting voxels using the p-value from the undadjusted linear model, excluding X_i . We thresholded the image based on a range of p values (0.05, 0.01, 0.001) and by taking a fixed number of voxels, ranked lowest to highest on p values (1000, 2000, 3000 voxels). For each patient scan, we calculated the percentage of voxels of the ROI that were classified as hemorrhage. Thus, if a patient's hemorrhage covered the entire ROI, the ROI coverage would be 100%. We then put this patient level ROI coverage into a linear regression model adjusted for the 3 confounders above:

$$Y_i = \beta_0 + \beta_1 \text{Coverage}_i + \gamma_1 \text{Age}_i + \gamma_2 \text{Gender}_i + \gamma_3 \text{TICHVol}_i + \epsilon_i$$

We computed another linear regression model replacing ROI coverage with a categorical indicator of the expert-specified ICH location classification, with categories: Thalamus ($N = 4$), Globus Pallidus ($N = 6$), Lobar ($N = 33$), and Putamen ($N = 68$). In order to determine whether using voxel level information improved prediction of functional score compared to standard hemorrhage classification we calculated a series of model-fit measures: R^2 , adjusted R^2 , Akaike information criterion (AIC) [1], and root mean squared error (RMSE).

ICH Localization and Engagement

As each patient's ICH mask are in MNI space, we can use previously segmented and labeled atlases of the brain to label spatial ICH engagement. We used the "Eve" atlas [28] to provide labeled regions. The Eve atlas was chosen because it segments and labels both gray matter (GM) and white matter (WM) regions. Ventricular regions are not explicitly segmented and categorized as background. We therefore modified the labels and categorized any region within the brain mask labeled as background in the Eve atlas as regions of cerebrospinal fluid (CSF), though this may encompass a small number of voxels that are not CSF.

We calculated the percent overlap of each hemorrhage mask with each labeled region of the atlas. That is, for each patient's ICH mask, we counted the number of voxels in each label of the Eve atlas, and then divided by the total number of voxels in the ICH mask to get the percent engagement for each region. These percentages represent a summary of region level engagement for each patient's ICH at a finer scale to coarsely classifying ICH engagement to only one region as done by readers. From these percentages, we can also calculate the region most engaged by the ICH for that patient similar to the categorization aforementioned done by experts. We did not directly compare reader-classified regions and the most-engaged region on the template as the template did not directly segment into the same categories used by readers for comparison.

Similar to the per patient scans, we calculated the percentage of engagement for the 3D histogram image based on the population, weighted by the proportion of patients with ICH at that location. Thus we can summarize a population of patients by a table of percentages of engagement with regions. Moreover, we can use prior anatomical and neurofunctional information to generate test hypotheses based on regions of the brain labeled by the atlas. We also calculated the percent engagement of regions for the best-performing ROIs for the NIHSS and GCS score analyses to characterize potential locations relating to these functional outcomes.

Results

Image Registration

The registered images for 2 patients are shown in Figure 3 with overlays (in pink) of the manually segmented blood in native space (panels a and d), the registered image and mask in template space

(panels b and e) and the overlaid mask onto the template (panels c and f). The slices are shown at the centroid (average location) of the hemorrhage mask. We chose one patient with variable slice thickness with a large hemorrhage (Figure 3a, b, and c) and one patient with a small hemorrhage (Figure 3d, e, and f). Images indicate that gross brain features remain relatively unchanged, but large deformations of tissue, mainly due to ICH, are preserved with registration. Also, we see the size of the registered brain in the patient with variable slice thickness is the same as the template, which implies the non-linear registration accounts for variable slice thickness, by non-uniform scaling.

[Figure 3 here.]

Histograms of ICH in the Brain

The histogram of the prevalence of hemorrhages over voxels (Figure 4a) shows the majority of voxels have a low prevalence; the median proportion of ICH at a given voxel is 3% ($N = 3$). We do observe that some voxels ($V = 5685$) have a high prevalence ($> 40\%$ of the sample), indicating similarities in areas of bleeding in this sample.

The resulting 3D histogram of the density of hemorrhages is shown in Figure 4b. In this image, voxels colored cooler (blue) correspond to a lower proportion of patients with hemorrhage at that voxel, whereas those colored hotter (red to yellow) correspond to a higher proportion. This histogram indicates that lesions are distributed medially in the brain in this cohort, with a lower concentration close to the cortical surface and higher in the left side of the brain. We see that some bi-laterality exists such that prevalence of ICH on left and right sides of the brain seem similar. Combining areas of engagement regardless of the side of the brain may be worthwhile, but combination of these areas is complicated by ICH that crosses the mid-sagittal plane. We do not see a high prevalence in the extreme anterior or posterior areas of brain. Nor do we see a high prevalence of bleeds in inferior areas of the brain, which is likely due to brain stems bleeds being excluded using the trial inclusion criteria.

These observations of ICH being centralized in the middle portion of the brain may also be an artifact of the inclusion criteria and may not generalize to other populations, but we note that no spatial location was preferred for inclusion. Regardless, creating these population images actually allows us to test if this location density does generalize to other populations given their density map.

[Figure 4 here.]

Prediction of Functional Score Based on Hemorrhage Location

We ran several versions of model (1) starting with the simplest case and then building the model by incorporating different choices of potential confounders to investigate their effects on the statistically significant association between ICH locations and functional score. More precisely, the five linear models are:

$$\begin{aligned}\mathcal{M}_1 : \quad & Y_i = \beta_0 + \beta_1(v)ICH_i(v) + \epsilon_{iv}, \\ \mathcal{M}_2 : \quad & Y_i = \beta_0 + \beta_1(v)ICH_i(v) + \gamma_1(v)Age_i + \epsilon_{iv}, \\ \mathcal{M}_3 : \quad & Y_i = \beta_0 + \beta_1(v)ICH_i(v) + \gamma_2(v)Gender_i + \epsilon_{iv}, \\ \mathcal{M}_4 : \quad & Y_i = \beta_0 + \beta_1(v)ICH_i(v) + \gamma_3(v)TICHVol_i + \epsilon_{iv}, \\ \mathcal{M}_5 : \quad & Y_i = \beta_0 + \beta_1(v)ICH_i(v) + \gamma_1(v)Age_i + \gamma_2(v)Gender_i + \gamma_3(v)TICHVol_i + \epsilon_{iv},\end{aligned}$$

where \mathcal{M} denotes a model. Also, we'll denote \mathcal{M}_6 as the voxel-wise Wilcoxon rank-sum test on functional score.

No voxels were significantly related to NIHSS score or GCS score in any model using the Bonferroni correction. We present maps of p-values for the models with NIHSS score as the outcome to potential areas of interest, as the Bonferroni correction is conservative and information can be gained at looking at the location of high and low p-values.

The p values for each model, with NIHSS score as the outcome, are presented in Figure 5, overlaid on a MRI T1 image for spatial localization of structures. The p values are colored with cooler (blue) colors representing higher p-values and hotter (red) colors representing lower p-values. Colors correspond to p-values .1 – 1 (dark blue), .1 – .05, (light blue), .05 – .01 (green), .01 – .001 (yellow), .001 – .0001 (orange) < .0001 (red). We see that there may be some relationship to medial hemorrhages with NIHSS score seen in the unadjusted model M_1 (Figure 5a) and the Wilcoxon rank-sum test (Figure 5f) and observe this when modeling the GCS score (Supplemental Figure 7). The p-values are higher in the models adjusted for age (Figure 5b), baseline ICH volume (Figure 5d), and both age and baseline ICH volume (Figure 5e). [Figure 5 here.]

Region of Interest Analysis

Figures 6a and 6b illustrate the voxels (in red) that were selected as the ROI based on p value or ranking of p-value for NIHSS and GCS score as the functional outcome, respectively. We observe that the ROIs appears larger on the left side compared to the right and many are near the ventricles, which may indicate ICH at these regions is important to functional score. We note that the ROI has spatial contiguity on either side of the brain, which is expected as the presence of ICH at a given voxel is highly correlated to that voxels neighbors. The number of voxels (V) for each p-value threshold (not displayed) were: .05 ($V = 47736$), .01 ($V = 19047$), .001 ($V = 2422$), which can correspond to rather large regions. As the resolution of the template is 1mm^3 , this corresponds to the ROI for a 0.05 p-value threshold measuring 48ml .

The corresponding number of voxels for p-value thresholds, using GCS as the functional outcome are: .05 ($V = 52368$), .01 ($V = 22858$), .001 ($V = 4669$), which again correspond to large ROIs for higher p-value thresholds.

Panels a and b of figure 6 show the unadjusted relationship of the percent ROI coverage with the functional score. We observe that the relationships are as expected, the larger the ROI coverage the higher (more severe stroke) NIHSS score and the lower (deeper unconsciousness) the GCS score.

[Figure 6 here.]

We present how these regions perform against using a location classification of ICH determined by readers. We summarized the model fit measures for in models for the NIHSS score (Table 2) and GCS score (Table 3). We have subtracted the AIC scores by the minimum value as these measures are unit less; the model with a value of 0 has the best (lowest) value for AIC.

We see that for NIHSS score, the ROI constructed using a p-value threshold of 0.0100 corresponded to the best model based on all our model fit measures. For the GCS score, the best model was one using an ROI using the voxels with lowest 1000 p-values. With respect to comparing model fit measures within models using the ROI coverage, all models due comparably well, defined as less than 5 unit difference in AIC, except for the ROI coverage model for ROI based on a p-value threshold of .05 modeling GCS score.

Though large differences in model fit measures using the ROI coverage are not observed, there is significant gain compared to using the reader classification with respect to R^2 . For the NIHSS models, the R^2 was 0.178 for the reader-classified location model compared to 0.282 for the best ROI coverage model, corresponding to a 58% relative increase. The result is similar when modeling GCS score: reader-classified location model $R^2 = 0.12$ vs best ROI coverage model $R^2 = 0.243$, corresponding to a 102% relative increase. Even though R^2 is relatively low for these models in absolute terms, the main goal of this ROI analysis was not prediction or model fit but rather comparison. We see that if these are potential goals for researchers, then using a CT-based measure can be potentially more informative than a reader-based categorical location predictor.

We observe larger gains for the ROI coverage model using adjusted R^2 , which penalizes the reader classified locations more than the ROI coverage model due to the additional predictors. Similarly, AIC would not choose the reader classified location model over any model using ROI coverage. Using the



~~RMSE as a criteria for model selection, the ROI coverage model outperform the reader classified location model.~~

[Tables 2 and 3 here]

Table 4 represents the beta coefficients from the models using reader-assessed location and the ~~ROI~~ coverage model ~~with the best model fit measures~~. The models for ~~ROI~~ coverage represent the best model based on the model-fit measures. We see that after adjusting for age, sex, and total baseline ICH volume, increasing 10% coverage is expected to increase NIHSS score by 2.0 (95% CI: 1.1, 2.8) points. We see that all locations, compared to lobar hemorrhages have higher estimated NIHSS scores, but putaminal hemorrhages were significantly higher by 4.2 (95% CI: 0.2, 8.2) points. Similarly for GCS score, adjusting for other covariates, increasing 10% coverage is expected to decrease GCS score by 0.4 (95% CI: 0.6, 0.2) points. All locations compared to lobar hemorrhages have lower estimated GCS scores, but none were statistically lower.

[Table 4 here]

ICH Localization and Engagement

Table 5 represents the 10 most-engaged regions for the population 3D histogram as well as the ROIs for the GCS and NIHSS score ROI analyses.

[Table 5 here]

Discussion

Semi-Automated Localization of ICH

We have characterized the localization of ICH in a population of stroke patients ~~within this~~ processing pipeline. We would like to stress that this is, as far as we know, the first 3D histogram of a population with ICH. We found that more patients had ICH engagement on the left side of the brain ~~compared to right~~ and both left and right sided ICHs are located towards the middle of the brain. The pipeline described is semi-automated allowing for more reproducible and objective analyses; the only non-automated steps in our pipeline are the ICH segmentation and export from OsiriX.

Voxel-wise Analysis of Functional Scores

Voxel-wise hypothesis tests were ~~calculated~~ using linear models or Wilcoxon rank-sum tests for NIHSS and GCS scores. The resulting p-values from these tests indicate that ICH at locations near the ventricles, particularly on the left side, may be related to functional scores. Although the voxel-wise regressions did not have any statistically significant results, this result is likely due to the strict threshold imposed by the Bonferroni correction. As each voxel is not independent of the other voxels as ICH is commonly a contiguous region of hemorrhage, this correction is inappropriate. Other methods that attempt to account of the smoothness properties, such as random field theory, may be more powerful. The voxel-wise analysis does provide a proof of concept and a screening procedure to generate a ROI for patient-level analysis.

Region of Interest Analysis

The region of interest analysis provides ~~some~~ evidence that using imaging-based location measures can result in better performance ~~when estimating~~ functional scores. Although ~~some measures were still relatively low with respect to model fit in absolute terms, such as an R^2 of 0.24~~, these measures showed demonstrable gains over using the reader-based categories commonly used in analysis.

This analysis focused on NIHSS and GCS scores as these were available at enrollment, but the process may be applied to long-term functional scores. As these populations had different interventions performed, we aimed to analyze outcomes that were prior to any separation of the groups induced by the trial.

Limitations

Although this set of patients represent a large proportion (79%) of the entire population ($N = 141$) of the MISTIE and ICES trials, the sample size is relatively small. This size was due to our selection process for scans and the number of patients available. The framework does not impose a restriction on the number of patients to be processed; it is extendable to much larger (hundreds or thousands) populations.

The current description of hemorrhages and all subsequent analyses are reliant on one specific registration technique. ~~If the registration is insufficient or poor, each patient's voxels are not spatially in the same location and aggregating over scans would not be appropriate or valid.~~ However, at this time the current software is the sole CT-only registration software and CT template published and available. ~~Though we have seen results indicating sufficient registration to the CT template, the template was made from healthy adults. Thus, brains with large deformations are registered to the template that was constructed from typical brains.~~ In future studies, ~~we may want to create a study-specific template for population-level analysis.~~ However, in that case, comparisons between analyses may be impossible as templates would change from study to study. Also, assessments of registration by visual inspection may be subjective.

~~The results from the ROI-based analysis are flawed in that the ROI has information based on the functional score by how they were generated.~~ Cross-validation can be used to split the data to a training group used to generate the ROI and a testing group to estimate model performance. ~~We plan to validate these ROIs on the subset of patients in the MISTIE and ICES trials not analyzed here.~~

Extensions of Analysis and Future Work

Although this analysis focused on patients from a single trial cohort, these tools can be applied to large-scale epidemiologic studies to better understand the ICH distribution in specific patient populations of interest and help predict patient outcomes. Moreover, this framework allows for the direct comparison of population-level ICH incidence between two populations. As each voxel represents a proportion, voxel-wise 2-sample proportion tests can be done.

Future research will focus on different registration techniques approaches and the variability of results conditional on the registration technique chosen.

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Tables

Variable (N = 111)	N (%) or Mean (SD)
Age in Years: Mean (SD)	60.8 (11.2)
Gender: Female	35 (31.5%)
NIHSS Score: Mean (SD)	22.1 (8.7)
GCS Score: Mean (SD)	10.0 (3.0)
Race	
Caucasian not Hispanic	59 (53.2%)
African American not Hispanic	35 (31.5%)
Hispanic	12 (10.8%)
Asian or Pacific Islander	5 (4.5%)
Reader-Classified ICH Location	
Putamen	68 (61.3%)
Lobar	33 (29.7%)
Globus Palidus	6 (5.4%)
Thalamus	4 (3.6%)

Table 1. Descriptive statistics of the demographic information on the patients.

Number of Voxels	P-value	Adjusted R ²	R ²	AIC	RMSE
Location Model		0.129	0.178	18.60	8.116
1000	0.0005	0.236	0.265	2.47	7.598
2000	0.0009	0.234	0.263	2.81	7.610
2422	0.0010	0.247	0.275	0.98	7.545
3000	0.0013	0.244	0.272	1.46	7.562
19047	0.0100	0.254	0.282	0.00	7.511
47736	0.0500	0.248	0.276	0.77	7.538

Table 2. Table of model-fit measures for NIHSS score: reader-based location model vs. CT voxel-based ROI coverage models. We see that the model using a p-value threshold of 0.0100 corresponds to the best model on all model-fit measures: adjusted and unadjusted R^2 are the highest; AIC, and RMSE are the smallest. The models using ROI coverage have comparable fit measures, but each ROI coverage model outperforms the reader-based location model, notably in the R^2 measures. Thus, we infer that using CT-based regions of interest may help in prediction of NIHSS score.

Number of Voxels	P-value	Adjusted R²	R²	AIC	RMSE
Location Model		0.069	0.120	20.51	2.914
1000	0.0002	0.214	0.243	0.00	2.677
2000	0.0004	0.213	0.242	0.09	2.678
3000	0.0006	0.212	0.241	0.25	2.680
4669	0.0010	0.212	0.241	0.23	2.680
22858	0.0100	0.191	0.221	3.17	2.716
52368	0.0500	0.166	0.197	6.44	2.757

Table 3. Table of model-fit measures for GCS score: reader-based location model vs. CT voxel-based ROI coverage models. We see that the model using a using the voxels with lowest 1000 p-values corresponds to the best model on all model-fit measures: adjusted and unadjusted R^2 are the highest; AIC, and RMSE are the smallest. The models using ROI coverage have comparable fit measures, but each ROI coverage model outperforms the reader-based location model, notably in the R^2 measures. Thus, we infer that using CT-based regions of interest may help in prediction of NIHSS score.

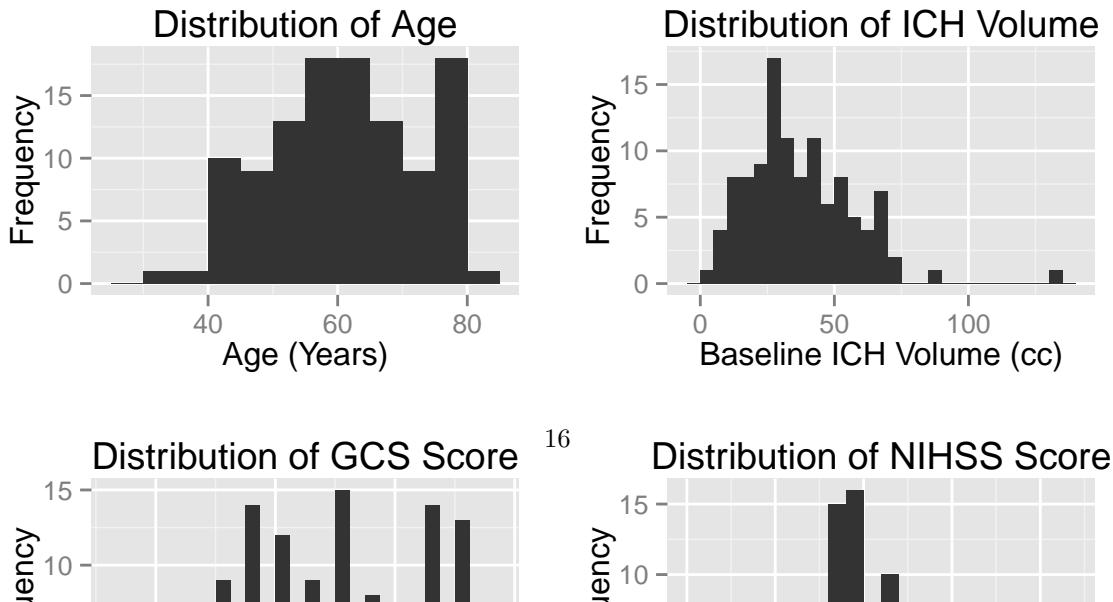
	NIHSS Score		GCS Score	
	ROI Coverage	Reader-Location	ROI Coverage	Reader-Location
Age	-0.04 (-0.2, 0.1)	-0.1 (-0.2, 0.1)	0.02 (-0.03, 0.1)	0.02 (-0.03, 0.1)
Sex: Male vs. Female	-0.7 (-3.8, 2.4)	-1.7 (-5.0, 1.7)	0.03 (-1.1, 1.1)	0.1 (-1.1, 1.3)
TICHVol per 10 cc	0.8 (-0.003, 1.5)	1.6 (0.8, 2.4)	-0.2 (-0.5, 0.02)	-0.5 (-0.7, -0.2)
ROI Coverage per 10%	2.0 (1.1, 2.8)		-0.4 (-0.6, -0.2)	
Reader-Based Location				
Globus Pallidus		4.5 (-2.9, 11.9)		-1.8 (-4.5, 0.8)
Putamen		4.2 (0.3, 8.2)		-1.2 (-2.6, 0.2)
Thalamus		4.8 (-4.1, 13.6)		-1.0 (-4.2, 2.1)
Constant	18.8 (9.1, 28.4)	19.6 (7.5, 31.7)	10.6 (7.4, 13.7)	11.2 (6.9, 15.5)

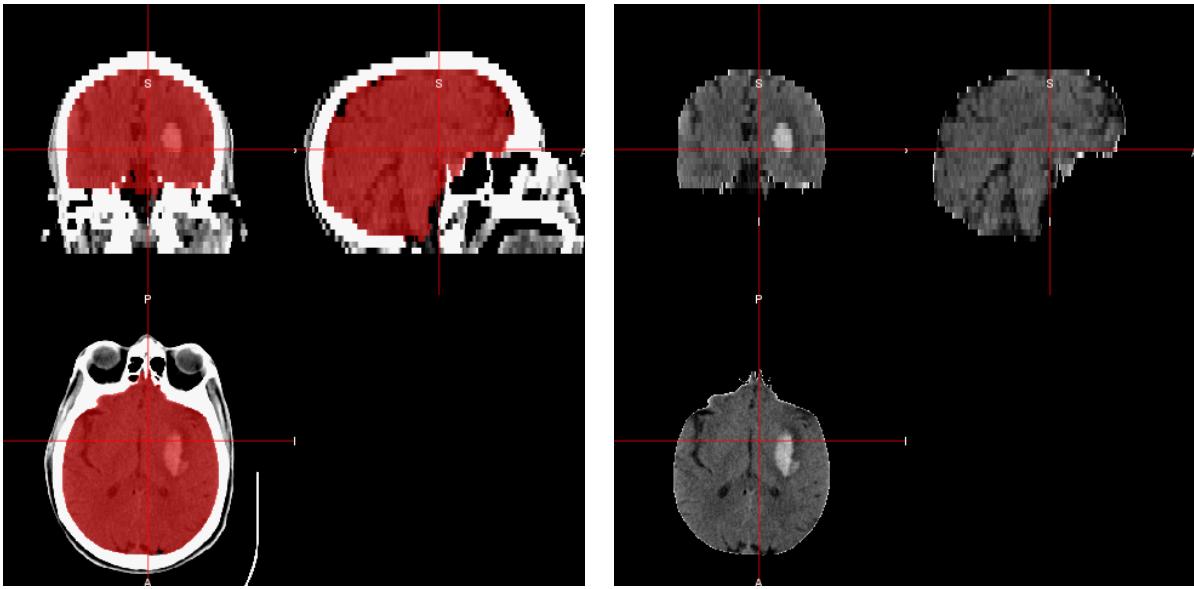
Table 4. Regression Models for ROI-Based Analysis. The models for ROI coverage represent the best model based on the model-fit measures. We see that after adjusting for age, sex, and total baseline ICH volume, increasing 10% coverage is expected to increase NIHSS score by 2.0 (95% CI: 1.1, 2.8) points. We see that all locations, compared to lobar hemorrhages have higher estimated NIHSS scores, but putaminal hemorrhages were significantly higher by 4.2 (95% CI: 0.2, 8.2) points. Adjusting for other covariates, increasing 10% coverage is expected to decrease GCS score by 0.4 (95% CI: 0.6, 0.2) points. We see that all locations, compared to lobar hemorrhages have lower estimated GCS scores, but none were statistically different.

Area	Population Prevalence	NIHSS ROI	GCS ROI
CSF	7.9	10.0	4.2
Insular	4.7		
Superior temporal gyrus	3.8		
Putamen left	3.0		
Insular right	2.9		
External capsule left	2.3		
Superior corona radiata left	1.9	11.8	27.9
Superior temporal wm left	1.9		
Superior corona radiata right	1.8		
Putamen right	1.8		
Posterior limb of internal capsule left		10.1	3.9
Thalamus left		7.6	33.9
Caudate nucleus left		5.4	9.6
Superior longitudinal fasciculus left		4.9	5.9
Globus pallidus left		3.7	
Anterior limb of internal capsule left		3.6	
Outside brain mask		3.5	
Anterior limb of internal capsule right		3.0	
Postcentral wm left			6.7
Posterior corona radiata left			3.1
Precentral wm left			1.3
Supramarginal wm left			1.1

Table 5. Distribution of the top 10 areas of engagement for population 3D histogram, the NIHSS ROI was based on a p-value threshold of 0.01, the GCS ROI was based on voxels with 1000 smallest p-values. Each value represents the percentage of the ROI engaged in this area. The population-level areas are percentages weighted by proportion. Each distribution of areas is based on the Eve atlas. We see that the population is engaged in areas of the CSF, such as the ventricles, and the insular and putaminal regions. The ROI based on the NIHSS analysis engages primarily areas of the internal capsule and ventricular regions. The ROI based on the GCS analysis engages primarily the left thalamus and superior corona radiata. The Eveatlas can be used to calculate area engagement on a per-scan level as well.

Figure Legends

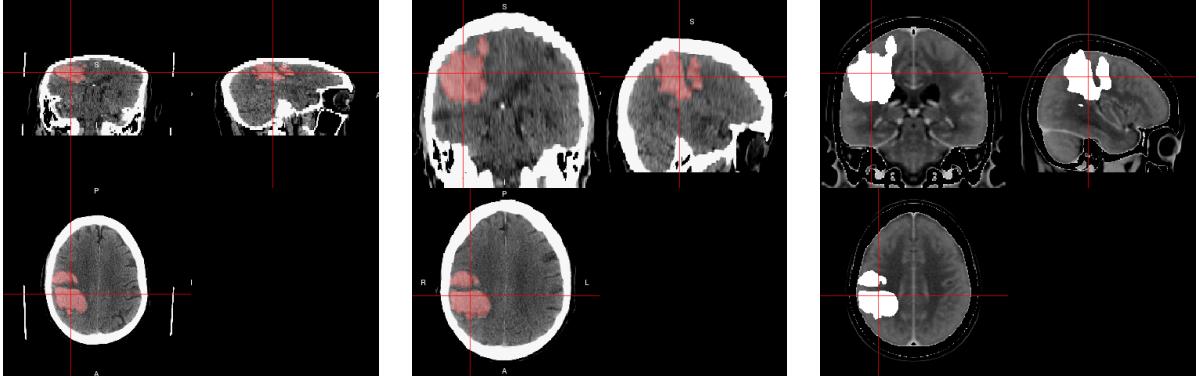




(a) Original Image (in native space) with overlaid brain-extraction mask colored in red. We observe that the mask does not appreciably drop out any areas of the brain nor does it add areas of the skull, eyes, or nose.

(b) Brain-extracted image used for re-centering to AC/PC line for SPM8 registration techniques.

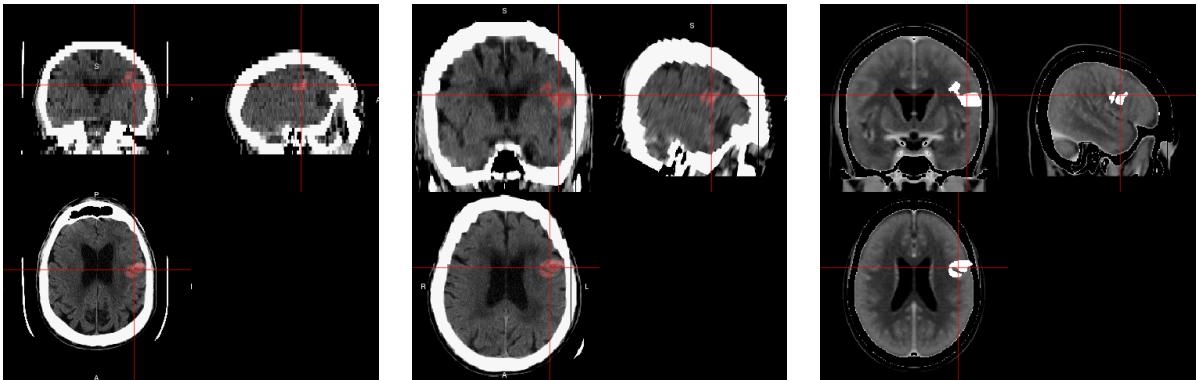
Figure 2. Image (a), displays the original image with the brain-extracted mask in red created from BET. Image (b) is the brain extracted image with the mask applied. We observe that the brain extraction appears to extract only the brain and not extra features. The image in (b) can be used for more quantitative patient-level measurements such as intracranial volume, mean Hounsfield units of areas, intensity-based normalization, and can restrict analyses to only brain tissue and not extracranial areas.



(a) Native space where the image looks “scrunched” vertically since the slice thicknesses are smaller for the middle and above part of the brain.

(b) Registered image with in template space with hemorrhage mask highlighted in pink. We observe that the brain has been stretched to match the dimensions of the template, yet structures on the patient image look to be in the same areas as that of the template in panel (c).

(c) Template image with hemorrhage mask overlaid in white.

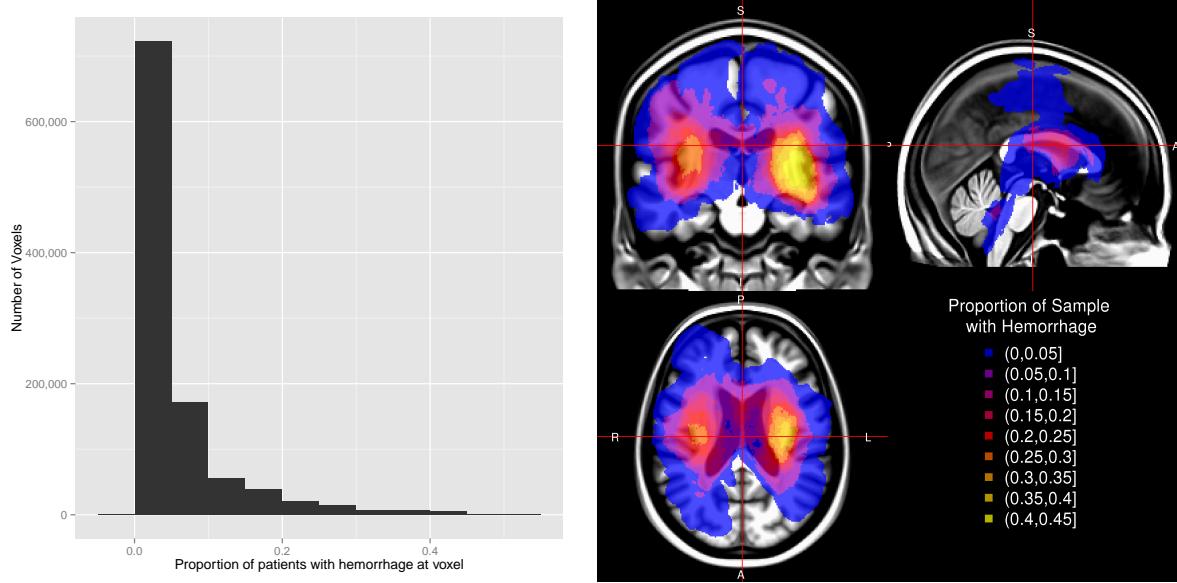


(d) Native space where image acquired with homogeneous slice thickness and a small ICH

(e) Registered image in template space with hemorrhage mask highlighted in pink. We observe the skull (in white) may be scaled during registration, but ventricles in the middle of the brain look similar to those on the template in panel (f).

(f) Template brain with hemorrhage mask overlaid

Figure 3. Native (left, panels (a) and (d)), template-registered (middle, panels (b) and (e)) images from two patients with template brain for comparison (right, panels (c) and (f)). In image (a) shows an image acquired with variable slice thickness, which can be seen as the top of the brain has smaller voxel sizes (thinner slices) than the bottom of the brain. We see in (b), the template-registered image, that the transformation has scaled the brain to the same size as the template. We see that similar structures, such as the lateral ventricles, are observed on the same axial slice on the patient-level scan compared to the template image, which indicates adequate registration. We observe a patient with a small ICH in panel (d), where we see the registration preserves the hemorrhage with respect to surrounding tissue, but may scale areas, such as the skull around the brain, too much.



(a) **Distribution** of proportion of patients with hemorrhage. All voxels with 0 proportion are excluded.

(b) **Template brain (MRI T1)** with proportion of hemorrhage overlaid

Figure 4. The histogram of proportion of patients for each voxel that had hemorrhage is presented in Figure (a). Voxels with 0 proportion are excluded. We observe the majority of voxels have a low prevalence, with a median of 3%, but some voxels ($V = 5685$) have a high prevalence of over 40% in this sample. In Figure (b), we present these proportions in a 3D histogram image (radiological convention - right side of image is left side of brain). Overlaid on the image is a MRI T1 template for spatial orientation and depictions of brain structures. Brighter values denote a higher percentage of patients that have a hemorrhage at that specific voxel. We see some bi-laterality of the image, but more hemorrhages in the left side of the brain compared to the right. ICH is also somewhat localized in the middle of the brain, with few extensions in the far anterior and posterior areas of the brain. The interactive version of this figure is located at http://muscellij2.github.io/CT_Pipeline/index.html.

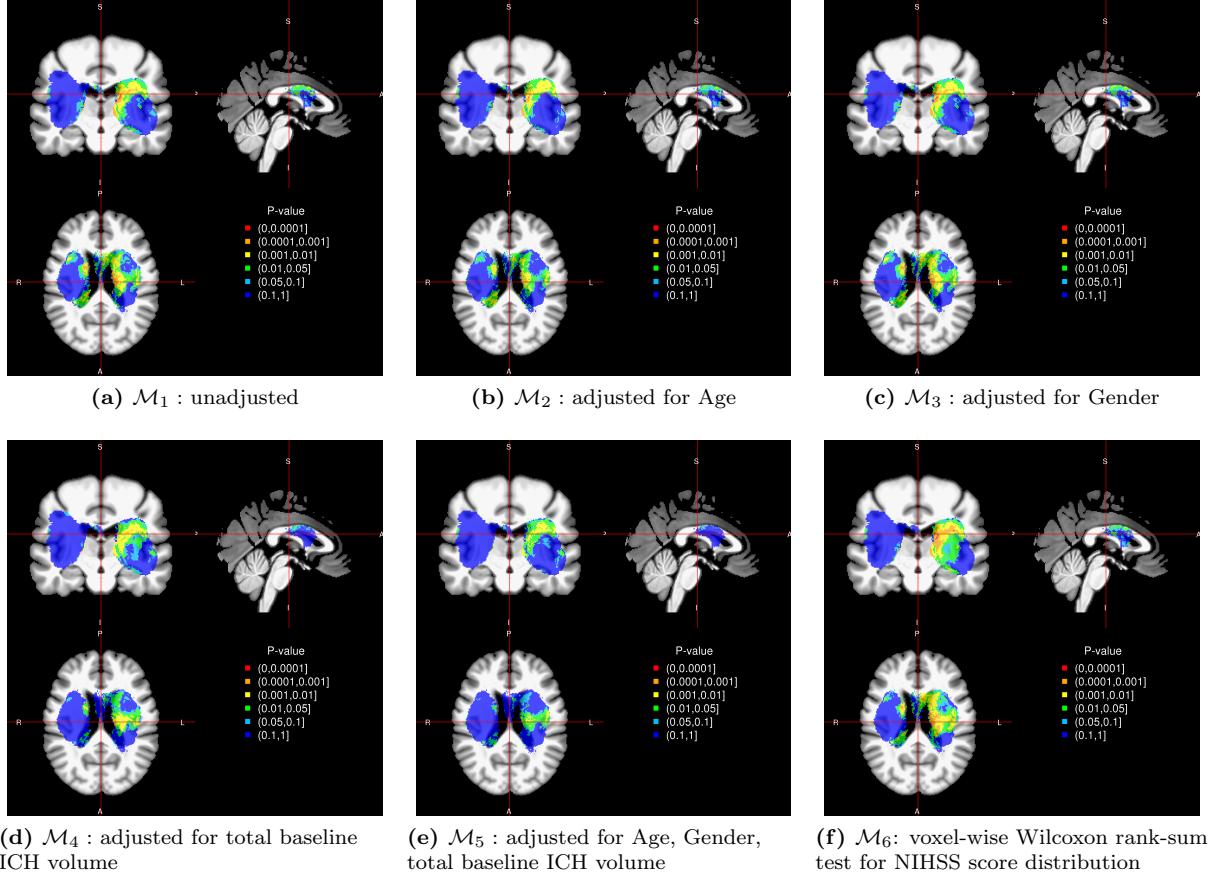
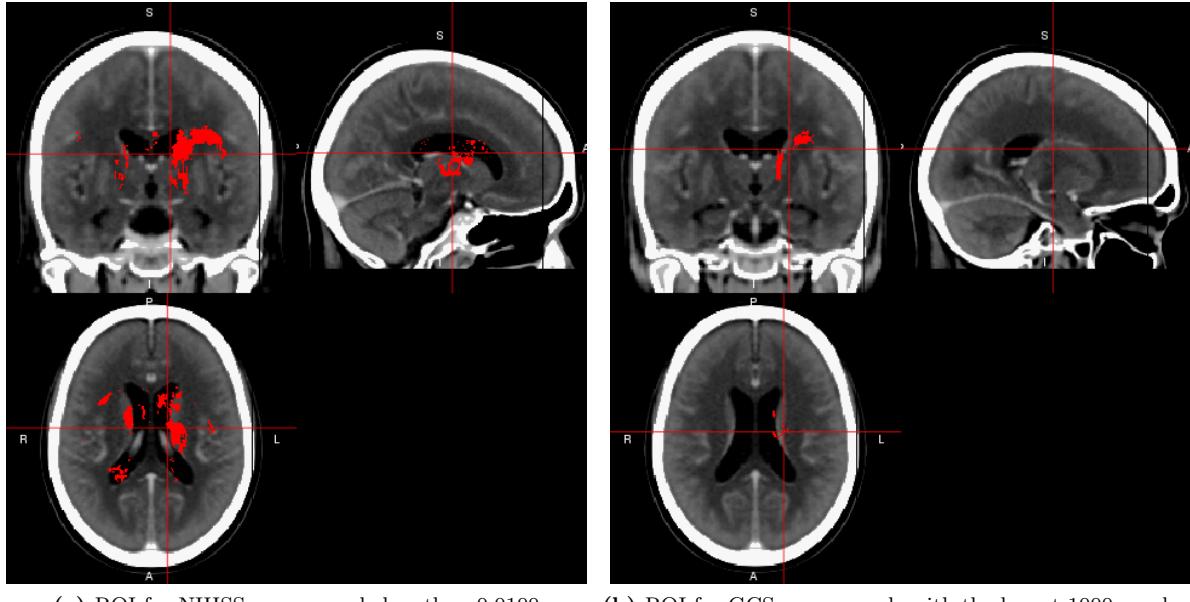
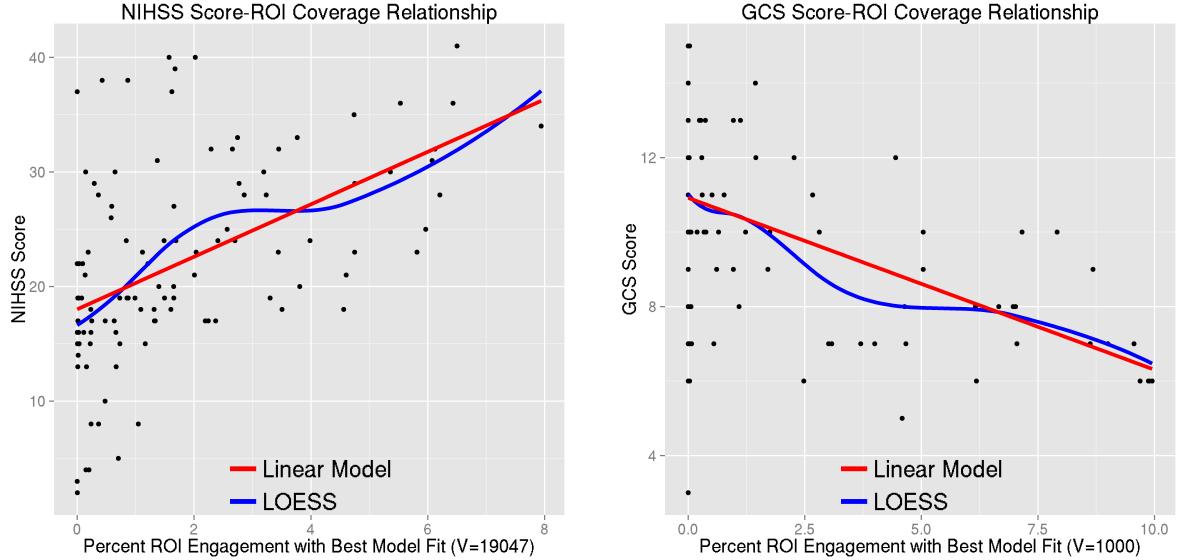


Figure 5. P-value maps for the 6 models, with NIHSS score as functional outcome. Colors correspond to p-values .1 – 1 (dark blue), .1 – .05, (light blue), .05 – .01 (green), .01 – .001 (yellow), .001 – .0001 (orange) < .0001 (red). We see that in the unadjusted linear model (panel (a)) and after adjusting for gender (panel (c)) there are voxels with the smallest p-values seem to be near the ventricles. In models adjusting for age (panel (b)), or total baseline ICH volume (panel (d)), or both (panel (e)), the p-value relating to NIHSS scores appear higher (more bluish). Also, we see the Wilcoxon rank-sum test have lower p-values for the same area compared to the unadjusted linear model (panel (f)). Slices are presented at the middle of the template.



(a) ROI for NIHSS score; voxels less than 0.0100

(b) ROI for GCS score; voxels with the lowest 1000 p-values



(c) Relationship of NIHSS score and ROI coverage for ROI in (a)

(d) Relationship of GCS score and ROI coverage for ROI in (b)

Figure 6. Region of Interest (ROI) Analysis. Panels (a) and (b) correspond to the ROI for the top-performing model for NIHSS and GCS scores, respectively. The ROI in panel (a) represents a p-value threshold of 0.0100 for the voxel-wise ICH on NIHSS score regressions, which includes 19047 voxels. The ROI in panel (b) represents 1000 with the lowest p-values for the voxel-wise ICH on GCS score regressions, corresponding to a p-value threshold of 0.0002. Panels (c) and (d) display the relationship of the ROI coverage to the functional score. The red line represents a linear fit (without adjustment of other covariates) of the ROI coverage and functional score and the blue line represents a LOESS fit. We see that the larger the ROI coverage the higher (more severe stroke) NIHSS score and the lower (deeper unconsciousness) the GCS score.

Supplemental Material

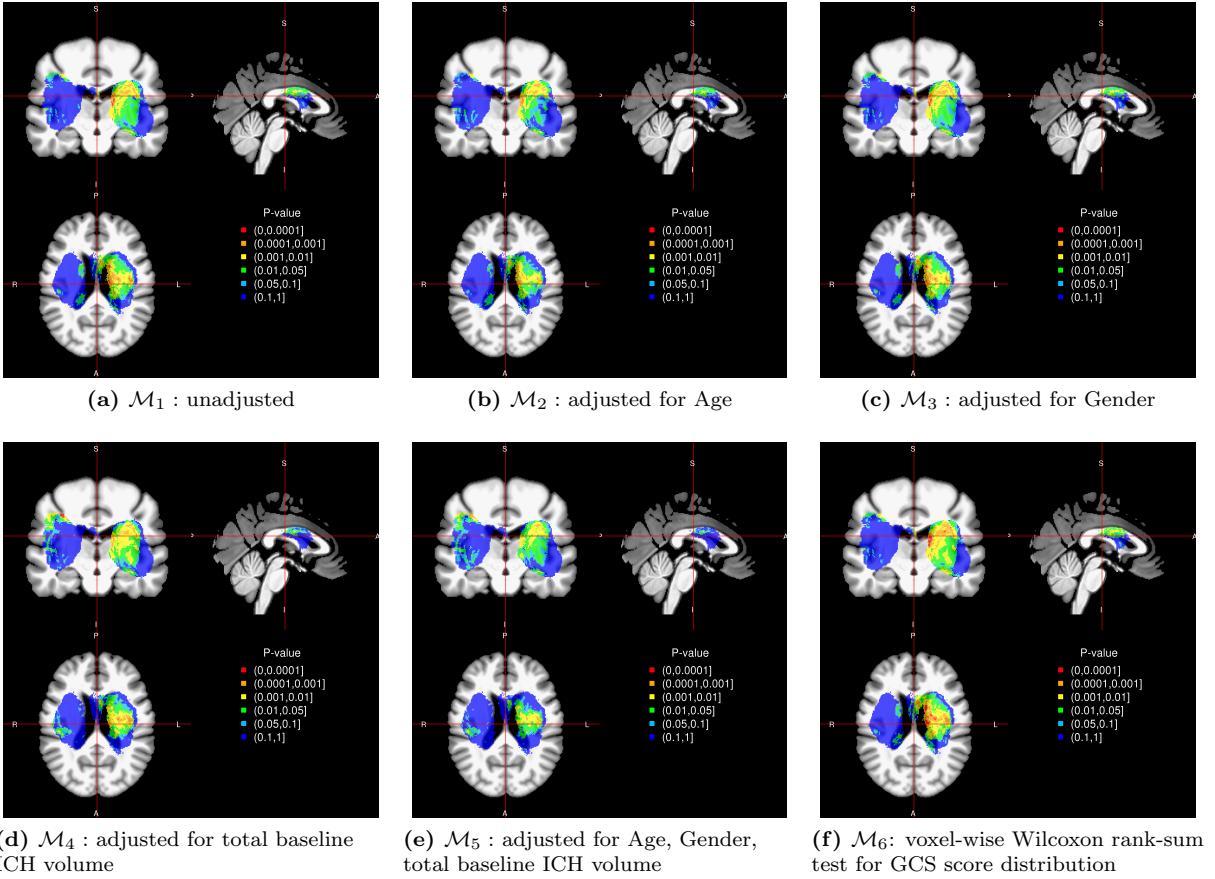


Figure 7. P-value maps for the 6 models, with GCS score as functional outcome. Colors correspond to p-values .1 – 1 (dark blue), .1 – .05, (light blue), .05 – .01 (green), .01 – .001 (yellow), .001 – .0001 (orange) < .0001 (red). We see that in the unadjusted linear model (panel (a)) and after adjusting for gender (panel (c)) there are voxels with the smallest p-values seem to be near the ventricles. In models adjusting for age (panel (b)), or total baseline ICH volume (panel (d)), or both (panel (e)), the p-value relating to GCS scores appear higher (more bluish). Also, we see the Wilcoxon rank-sum test have lower p-values for the same area compared to the unadjusted linear model (panel (f)). Slices are presented at the middle of the template.