The map Ru can be identified with a matrix

Re= (Ri) E Rkmxn

where R,,..., R, E IR are the projection matrices of individual X-ray illuminations.

Unlike in [Burger et al, 2021], let us assume that the projection geometries for R1,..., Rx are fixed. Let us also assume that the unknown pixelwise absorption values are modeled as a random vector X ∈ R" with a Gaussian (prior) distribution, X ~ N(xpr, Tpr), and that the measurement model is belongs to prior

 $Y = \Re_{k}X + N$ 

where the additive noise N is indpendent of X and follows a zero-mean Gaussian distribution, Nr W(0, Mosse).

Under these assumptions, the posterior distribution of X, given a realized measurement y = Y, is  $X \mid y \sim \mathcal{N}(x_{post}, \Gamma_{post})$ , where

(\*)  $\Gamma_{post} = \Gamma_{pr} - \Gamma_{pr} \mathcal{R}_{k}^{T} (\mathcal{R}_{k} \Gamma_{pr} \mathcal{R}_{k}^{T} + \Gamma_{noise}) \mathcal{R} \Gamma_{pr},$   $\times_{post} = \times_{pr} - \Gamma_{pr} \mathcal{R}_{k}^{T} (\mathcal{R}_{k} \Gamma_{pr} \mathcal{R}^{T} + \Gamma_{noise}) (y - \mathcal{R}_{k} \times_{pr}).$ 

The idea of Bayesian experimental design is to make Tpost "as small as possible" in a certain sense. In your thesis the preferred measure of "smallness" is the A-optimality criterion measured by the A-optimality target function

P<sub>A</sub>(d) = tr (AΓ<sub>post</sub>(d) A<sup>τ</sup>), A∈ R<sup>n×n</sup>,

where d∈ R<sup>q</sup> is the design parameter

and A is a predetermined weight matrix

that can, e.g., define a region of interest

inside the examined domain. If A is

the iduntity matrix, then Φ<sub>A</sub> measures the

expected squared reconstruction error, i.e.,

IE(1X-×<sub>post</sub>1<sup>2</sup>), where 1.1 denotes the Euclidean

x

From (\*) it is rather obvious that the minimizer of  $\Phi_A$  without any extra constraints is d=0. This would mean minimizing noise without any restrictions on the radiation dose.

Let us assume that the radiation (4) dose is inversely propotional to the Variance of noise, i.e.,

dose; = 
$$\frac{c}{d_i^2}$$
,

where c>o is a positive constant. (I am not sure how physically accurate this model is, but at least it has a suitable behavior for our purposes.)

The assumption is that the overall dose is not allowed to exceed some predefined limit, say, D > 0.

The complete minimization task thus

$$d^* = argmin(tr(ATpost(d)AT), [probably continued])$$

$$\lim_{j=1}^{km} \frac{1}{d_j^2} \leq \frac{D}{C},$$

$$\lim_{j=1}^{km} \frac$$

The main steps are (approximately) as follows:

- 1. Try to understand these notes and the relevant parts of [June] [Burger et al, 2021] and the program codes I sent you.
- 2. Deduce the gradient (and possibly) also the Hessian of the target [June] function \$\Phi\_A(d)\$ with respect to d. Help can be found, e.g., in the master's thesis of Jamo Maaninen.
- Consider techniques of constraint optimization and choose suitable [June] ones for tackling (t). (Material will be provided a bit later.)
- 4. Implement the algorithm and test it with some sets of since [June & July] settings in the spirit of the provided codes.
- Louly 5. Write the thesis. & August (