Zero-shot classification of ECG signals using a CLIP-based model

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Keywords: keyword1, keyword2, keyword3, keyword4, keyword5. (Min.5-Max. 8)

Abstract

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# Introduction

According to the World Heart Federation (WHF), prominent medical institutions, and leading healthcare professionals, cardiovascular diseases (CVDs) are a leading cause of mortality worldwide [17; 22; 25; 36]. In the United States, the Center for Disease Control (CDC) estimates that the annual total cost associated with CVD-related treatment and mortality is approximately $219 billion dollars (USD) per year [18; 21]. Given the significant financial and socioeconomic burdens of CVDs, it is essential that individuals receive timely and accurate medical care for the diagnosis, treatment, and ongoing care of CVDs.

The electrocardiogram (ECG) remains the medical standard and benchmark for the identification and diagnosis of CVDs with more than 300 million ECGs being performed globally [7]. An ECG measures the changes in electrical membrane potential of the heart across different directions of the body and are often referred to as leads with a 12-lead ECG report being the most common type of ECG clinical report [14; 29]. Once an ECG report is available, it is then analyzed by a licensed medical professional such as a cardiologist or an auxiliary medical professional.

Interpreting and analyzing ECG reports remains a highly complex and time-consuming process for medical professionals [11]. This process not only requires manual annotation of ECGs but also mandates that the individual analyzing the ECG possesses a vast understanding of topics such as cardiac anatomy, electrophysiology, pattern recognition, coronary distribution, and pathophysiology to perform correctly and accurately [11]. A systematic literature review by Cook et al. revealed that medical professionals, such as cardiologists, across levels of education experienced challenges in providing a correct diagnosis for an ECG report with correct interpretation accuracy ranging from 49% to 92% and with a median interpretation accuracy of 57% [11]. The review also found that medical professionals who received continuing education and training improved their ability to correctly provide a diagnosis for an ECG report with a median accuracy of 67%, underscoring the importance of continuous professional development in ECG interpretation [11].

Recognizing the challenges in ECG interpretation faced by medical professionals, researchers have turned to advancements in machine learning (ML), deep learning (DL), and artificial intelligence (AI) to address this issue. Namely, with the numerous advancements observed in ML, DL, and AI vision models over recent years, it was postulated that ML and DL vision models could accurately classify pathologies from ECG reports.

In this paper, we aim to advance the field of deep learning (DL) as it pertains to ECG classification. Specifically, we demonstrate the effectiveness of using a multimodal Contrastive Language-Image Pre-training (CLIP) framework for diagnosing various combinations and permutations of ECG diagnostic classes. Our literature review indicates that the application of a multimodal CLIP framework in ECG classification has been minimally explored, with only a few studies published in the past two years.

In the next section, “Related Works,” we provide an overview of CLIP and the current state of ML and DL models for ECG classification. Additionally, we discuss Zero-shot classification as it relates to our study.

# Related Works

## Contrastive language image pre-training (CLIP)

In 2021, OpenAI researchers published their paper, “Learning Transferable Visual Models From Natural Language Supervision” which introduced a novel approach to multimodal learning, namely, Contrastive language image pre-training or CLIP for short [10; 20]. CLIP is a multimodal framework that comprises of two components, an image encoder (vision model) and a text encoder (text model) [10; 20]. When using a CLIP framework, the image encoder is trained alongside the accompanying text encoder [10]. This allows the CLIP-based model to develop a comprehensive or "deep" understanding of its image-text pair inputs [20]. To facilitate the learning process, the CLIP framework utilizes contrastive loss (also known as symmetric loss) [10; 20]. Contrastive loss calculates the distance between the embeddings of the image-text pair inputs and aims to minimize the overall distance between image-text pairs when one sample is like another (positive instance) and maximize the distance between image-text pairs inputs when samples are not similar to other samples (negative instance) [10; 20]. In doing this, the two text and image encoders are incentivized to learn better representations of their inputs to capture the semantic relationship between embeddings of image-text pairs and are penalized when they do not learn or capture reliable representations of the image-text pairs [20].

Unlike traditional ML or DL approaches for classification tasks, which are generally jointly trained with some image feature extractor and a classifier to predict the corresponding image class or label(s), the notion of using a CLIP-based model presents a novel approach for classification tasks [20]. With a CLIP-based model, the model can be utilized for zero-shot classification across a variety of classification tasks and for many types of datasets. In our study, we demonstrate that a CLIP-based model can be used within zero-shot learning (pending).

Task 1: Put Image of Contrastive Learning Pseudocode or type in LaTex and insert equations

## Related Works – Deep Learning and ECG Classification

In the fields of AI, ML, and DL, the primary goal has been to create models capable of correctly classifying CVDs from ECG reports [2]. To achieve models capable of this, a patient’s medical history including their ECG report(s) are aggregated, preprocessed, and then analyzed by the model which in the end, provides a recommendation or classification based on its input.

In the past decade, several notable ECG classification models have been developed that have demonstrated to be as effective in correctly classifying CVDs from ECGs as experienced cardiologists using ECG signal inputs [4; 23]. In one systematic literature review about state-of-the-art (SOTA) DL methods for ECG classification by Petmezas and colleagues, it was found that the most popular DL models for ECG classification tasks included variants of convolutional neural networks (CNNs), recurrent neural networks (RNNs), ResNet models, and LSTM models [33]. From the studies reviewed in this systematic review, 66.1% favored using CNNs for specific, downstream ECG classification tasks [33]. In Lu et al.’s study, the researchers achieved an accuracy of 99.31% for arrhythmia classification using a 1D-CNN [19; 33]. In a different study, authors Yu et al. achieved an accuracy of 99.70 % for premature ventricular contraction also utilizing a 1D-CNN demonstrating the robustness of CNNs for different types of, singular-class of ECG classification tasks [6; 33]. Other studies have also demonstrated that training and using CNNs is effective for CVD classification tasks for classes such as myocardial infarction, coronary artery disease, and congestive heart failure to name a few.

## Related Works – CLIP-based models in medical imaging

Using a CLIP-based model has proven to be effective across a wide range of datasets and classes such as s Food-101, CIFAR-100, ImageNet, and MNIST to name a few [20]. However, the utilization of CLIP-based models in medical imaging for image classification or diagnostic tasks remains an area of research that has not been analyzed or explored extensively [9]. In their systematic literature review on the topic of CLIP-based models for medical imaging, Zhao et al. found that since 2021, there have been approximately 38 studies that have utilized the CLIP-based model framework for medical imaging tasks [9]. From these 38 studies, some notable examples include seven studies using the CLIP-based framework for the classification of chest X-rays, one study using the CLIP-based framework for the stomach histology, one study for CT scans of the lungs, one study for the classification of skin/dermatology conditions, one study for MRIs of brains, and one study used the CLIP-based framework for eye classification tasks [9].

In Zhao et al.’s systematic review, there was only one study that used the CLIP-based framework for ECG classification tasks which used ECG signals as their primary input [9; 15]. In their paper, "ETP: LEARNING TRANSFERABLE ECG REPRESENTATIONS VIA ECG-TEXT PRE-TRAINING", authors Liu et al. describe training a CLIP-based model from scratch using the PTB-XL and CPSC2018 datasets [3; 15; 30]. In this study, 12-lead ECG reports and their corresponding ECG signals were used to train a CLIP-based model where a 1D-ResNet18 model served as the image encoder and BioClinicalBERT was used as the text encoder [15; 31]. During the training of the image encoder, the 1D-ResNet18 model had its weights updated during training whereas the text encoder, BioClinicalBERT, had its weights remain constant or frozen [15]. The aim of Liu et al.’s study was to demonstrate the viability of zero-shot ECG classification tasks [15]. In their experiments, the joint multimodal training of image and text encoders simultaneously achieved SOTA results for ECG classification on the PTB-XL and CPSC2018 datasets, respectively, during both supervised learning as well as during zero-shot classification [15]. In the PTB-XL zero-shot classification experiment, their ETP model achieved higher AUC, ACC, and F1 scores across four distinct classes of ECGs [15]. Similarly, their ETP approach also achieved significant results on the CPSC2018 dataset achieving higher AUC, ACC, and F1 scores across nine distinct classes of ECGs [15]. Both experiments demonstrated the robustness of using the CLIP-based framework for ECG classification in both supervised learning and zero-shot learning/classification [15]. Liu et al.’s study was important because it was the first study that demonstrated that the CLIP framework could be used for zero-shot classification of ECGs and in this study, we aim to build on their work across a greater number of ECG diagnostic classes and larger datasets.

Another study that demonstrates the efficacy and value of multimodal or joint training of image and text encoders was seen in Li et al.’s, "Frozen Language Model Helps ECG Zero-Shot Learning" [16]. In this study, the authors introduced a new technique called Multimodal ECG-text SSL or METS for short [16]. Like Liu et al.’s study, Li et al. in their study also use a text encoder with frozen weights where the goal of METS is to use automatically generated ECG clinical reports to guide the training of the ECG image encoder [15; 16]. The METS approach achieved an improvement of 10% in performance without the use of annotated datasets relative to comparable studies in this field [16].

In summary, the METS model takes an ECG signal and its corresponding ECG report/diagnosis text as inputs and feeds them into a multimodal learning framework, like CLIP [16; 20]. Then, using contrastive loss, they attempted to measure the distance between image-text pairs so that their ECG image encoder can learn "deep" representations of its 9 inputs [16]. When it came to evaluation, the METS approach achieved higher accuracy, precision, recall, and F1 scores in the PTB-XL compared to other leading methods [16].

## Related Works – Zero-shot Learning

* Task: Need specific articles that describe Zero-Shot Learning

According to Hugging Face, zero-shot classification is a natural language processing (NLP) task where a model is trained on a specific set of labeled image-text pair data but can generalize and classify new examples of classes that were not in the labeled image-text pair dataset during the model’s training [38]. In this study, a simple example of zero-shot classification would be if the image model were trained on a set of labeled image-text pairs with some classes of image-text pairs that were excluded during training (for example, ECG signals for myocardial infarction). Then, during the testing phase, the trained image model would be able generalize to new data and in turn be able to classify myocardial infarction.

# Materials and Methodology

## Datasets

Two experiments were performed in this study, Experiments A and B, respectively.

### Datasets – Experiment A

In Experiment A, a CLIP-based model consisting of a text encoder and image encoder, was trained on the Physikalisch-Technische Bundesanstalt (PTB-XL) dataset. The PTB-XL dataset contains ECG image-text pairs where each image is represented by a raw 10 second 12-lead ECG signal and where the ECG clinical report represents each text input. In Experiment A, the CLIP-based model was trained on most of all classes in the PTB-XL dataset with some exceptions. Those classes which were excluded during the training of the CLIP-based model were utilized for the testing and evaluation of the CLIP-based model where the CLIP-based model would encounter ECG diagnostic classes that it had not previously encountered or seen during its training. In doing this, the CLIP-based model could be evaluated in a zero-shot classification setting to determine how well the CLIP-based model is able to generalize to unseen data.

excluded\_classes = ['left ventricular hypertrophy',

'st depression',

'low qrs voltages',

's t changes',

'sinus tachycardia',

't wave abnormal',

'right axis deviation']

**Figure 1**: Distribution of Classes (labels) in the PTB-XL dataset

|  |  |
| --- | --- |
| **Diagnostic Class** | **Total Samples** |
| sinus rhythm | 18058 |
| myocardial infarction | 5248 |
| left axis deviation | 5146 |
| abnormal QRS | 3389 |
| left ventricular hypertrophy | 2354 |
| t wave abnormal | 2341 |
| myocardial ischemia | 2171 |
| left anterior fascicular block | 1624 |
| atrial fibrillation | 1514 |
| ventricular ectopics | 1153 |
| incomplete right bundle branch block | 1118 |
| st depression | 1009 |
| sinus tachycardia | 826 |
| 1st degree av block | 795 |
| nonspecific intraventricular conduction disorder | 787 |
| sinus arrhythmia | 772 |
| s t changes | 768 |
| sinus bradycardia | 637 |
| qwave abnormal | 548 |
| complete right bundle branch block | 542 |
| left bundle branch block | 536 |
| left atrial enlargement | 426 |
| premature atrial contraction | 398 |
| nonspecific st t abnormality | 381 |
| anterior myocardial infarction | 353 |
| right axis deviation | 343 |
| prolonged pr interval | 340 |
| t wave inversion | 294 |
| pacing rhythm | 294 |
| inferior ischaemia | 218 |
| low qrs voltages | 182 |
| left posterior fascicular block | 177 |
| supraventricular premature beats | 157 |
| indeterminate cardiac axis | 155 |
| lateral ischaemia | 140 |
| right ventricular hypertrophy | 126 |
| prolonged qt interval | 118 |
| right atrial hypertrophy | 99 |
| ventricular bigeminy | 82 |
| wolff parkinson white pattern | 79 |
| incomplete left bundle branch block | 77 |
| atrial flutter | 73 |
| anterior ischemia | 44 |
| ventricular hypertrophy | 29 |
| st elevation | 28 |
| supraventricular tachycardia | 27 |
| paroxysmal supraventricular tachycardia | 24 |
| ventricular trigeminy | 20 |
| complete heart block | 16 |
| 2nd degree av block | 14 |

### Datasets – Experiment B

In Experiment B, the primary dataset used was the [insert dataset here, subject to change].

## Data pre-processing

In Experiments A and B, the raw ECG signal for each ECG image-text pair was down sampled from its original frequency to 128 Hz. After down sampling the ECG signals, the ECG signals were then normalized by calculating the average mean and average standard deviation for all samples. The down sampled dataset is then filtered to exclude any diagnostic classes with fewer than 100 samples to ensure that sufficient data was available to train the models in both experiments.

## Model architecture

### Text Encoder – BioClinicalBERT

In Experiment A, the text encoder used as part of the CLIP-based model was BioClinicalBERT. BioClinicalBERT is a variant of the BioBERT base model which is additionally trained on all notes from MIMIC III, a database of electronic health records from ICU patients at Beth Israel Hospital in Boston, MA and which contains over 880 million words [31]. The pretrained BioClinicalBERT is publicly available through HuggingFace.

The implementation of the BioClinicalBERT text encoder in Python3 can be seen in the Figure below.

* Task: For LaTex, insert code correctly within a code block.

### Image Encoder – 1D-CNN or [SOME OTHER MODEL, TBD]

## Model training

In Experiment A, the CLIP-based model consisting of a 1D-CNN image encoder and the BioClinicalBERT text encoder was trained and validated on the PTB-XL dataset. The CLIP-based model was trained over 20 epochs with a learning rate of 0.001, Adam optimizer, a StepLR scheduler,

**Table 1:** Hyperparameters for Experiment A

|  |  |
| --- | --- |
| **Hyperparameter Type** | **Value** |
| Epochs | 20 |
| Optimizer | torch.optim.Adam |
| Projection Dimension | 64/128/256/512/768/1536 |
| Projection Head Learning Rate | 0.001 |
| Image Encoder Learning Rate | 0.001 |
| Image Encoder Type | 1D-CNN |
| Text Encoder Type | BioClinicalBERT |
| Temperature | 1.0 |
| ECG Signal Sample Rate (Hz) | 128 |
| Dropout | 0.0 |
| Criterion (Loss Function) | Contrastive Loss |

**Table 2:** Hyperparameters for Experiment B

|  |  |
| --- | --- |
| **Hyperparameter Type** | **Value** |
|  |  |

* Task: Create LaTex tables for Tables 1 and 2.

# Results

### 4.1 Results – Experiment A

The trained CLIP-based model demonstrated good performance during the training and validation phases. Over 20 epochs, the CLIP-based model achieved average AUC-ROC scores of 0.711 and 0.721 on the training and validationdata subsets. In addition, the average AUC-PR scores achieved were 0.073 and 0.073 on the training and validationdata subsets. The average accuracy score across all dataset labels in the training and validationdata subsets was 0.188 and 0.165, respectively. It was observed that class labels with a greater number of samples achieved higher scores across the evaluation metrics whereas class labels with fewer samples did not achieve high scores in evaluation metrics. A full summary of these results is summarized [here](https://github.com/naavie/Scientific-ECG-PUBLIC/blob/main/Experiment%20A/expA_history_256%20(1).csv).

When the trained CLIP-based model was evaluated on unseen classes of ECGs, it was observed that performance was poor suggesting that the model was struggling to generalize to unseen data.

### 4.2 Results – Experiment B

In Experiment B, the same image encoder from the CLIP-based model was trained on the Georgia dataset. A summary of the baseline results can be found here (hyperlink needed)

The trained CLIP-based model from Experiment B performed

# Discussion

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