Supporting information for:

Investigating the Impact of Network Functionalization on Protein Adsorption to Polymer Nanogels

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1. Theoretical Method

1.1. Molecular Theory

In this section, we describe the molecular theory used in this work. The same formalism can be applied to various different systems. Here we are particularly interested in its is application to describe the adsorption of some proteins of interest to nanogels made of copolymer chains of ionizable and hydrophilic monomers.

The system under study is a single nanogel in equilibrium with an aqueous solution having externally defined bulk composition. The pH, salt concentration and protein concentration of this solution are the independent variables. The polymer network that gives structure to the nanogel contains two types of segments: a pH-sensitive unit, either acidic (MAA) or basic (AH), and a neutral segment (VA); crosslinks are described as charge neutral segments.

The semi-grand potential of our system contains the following contributions:

$$\Omega_{NG} = -TS_{mix} - TS_{conf,nw} + F_{chem,nw} + F_{chem,pro}
+ U_{elec} + U_{ste} + U_{vdw} - \sum_{\gamma} \mu_{\gamma} N_{\gamma} - \mu_{pro} N_{pro}$$
(1)

Next, we will provide the explicit form of each of these terms for the particular case where methacrylic acid (MAA) is the protonable segment. However the same or analogous expressions apply for networks having basic segments.

In Eq. (1), the translational and mixing entropy of the mobile species (including the protein) is

$$\frac{S_{mix}}{k_B} = -\sum_{\gamma} \int_0^\infty dr G(r) \rho_{\gamma}(r) \left(\ln \left(\rho_{\gamma}(r) v_w \right) - 1 + \beta \mu_{\gamma}^0 \right) \\
- \sum_{\alpha} \int_0^\infty dr G(r) \rho_{pro}(\theta, r) \left(\ln \left(\rho_{pro}(\theta, r) v_w \right) - 1 + \beta \mu_{pro}^0 \right)$$
(2)

where $\beta=\frac{1}{k_BT}$, k_B is the Boltzmann constant, v_w is the volume of a water molecule, and T is the temperature of the system. Radial coordinate r measures the distance from the center of mass of the polymer network. $\rho_{\gamma}(r)$ and μ_{γ} are respectively the local number density and the chemical potential of free species γ , where subindex γ runs over water molecules and its ions (hydronium and hydroxyde), and the salt dissociated ions (Na^+ , Cl^-). $G(r)=4\pi r^2$ is the surface area of the sphere of radius r, which results from integrating out the angular component of the volume element when incorporating the radial symmetry of our problem.

The entropy of mixing, Eq. (2), also includes contributions for the protein. μ_{pro}^0 is the standard chemical potential of the protein. $\rho_{pro}(\theta,r)$ is the local density of the protein in conformation θ . These conformations also include spatial rotations. Then, the total local density of proteins is:

$$\langle \rho_{pro}(r) \rangle = \sum_{\theta} \rho_{pro}(\theta, r)$$
 (3)

 $S_{conf,nw}$ in Eq. (1) represents the conformational entropy that results from the flexibility of the polymer network, which can assume many different conformations denoted by the set $\{\alpha\}$.

$$\frac{S_{conf,nw}}{k_B} = -\sum_{\alpha} P(\alpha) \ln P(\alpha)$$
 (4)

where $P(\alpha)$ denotes the probability that the nanogel network is in the configuration α . A network conformation is specified by the position of all its segments. The volume fraction of these segments can be expressed as

$$\langle \phi_i(r) \rangle = \sum_{\alpha} P(\alpha) \phi_i(\alpha, r)$$
 (5)

Subscript i indicate the segment type (i = MAA/VA/crosslink), and angle brackets denote an ensemble average over network conformations. $\phi_i(\alpha, r)$ is an input quantity that gives the local volume fraction occupied by i-type segments at r, when the network is in conformation α .

The next term in Eq. (1) describes the free energy of the acid-base equilibrium. For MAA segments:

$$\beta F_{chem,nw} = \int_0^\infty dr G(r) \frac{\langle \phi_{MAA}(r) \rangle}{v_{MAA}} \left[f(r) (\ln f(r) + \beta \mu_{MAA^-}^0) + (1 - f(r)) (\ln (1 - f(r)) + \beta \mu_{MAAH}^0) \right]$$

$$(6)$$

where f(r) is the degree of charge of MAA segments when they occupy the spherical shell between r and r+dr. $\mu^0_{MAA^-}$ and μ^0_{MAAH} are the standard chemical potentials of the deprotonated and protonated species respectively. v_{MAA} is the molecular volume of the MAA segment.

Similarly, the chemical equilibrium of titratable units of the protein is accounted for in the following free energy term:

$$\beta F_{chem,pro} = \int_0^\infty dr G(r) \sum_{\tau} \left\langle \rho_{pro,\tau}(r) \right\rangle \left[g_{\tau}(r) (\ln g_{\tau}(r) + \beta \mu_{\tau p}^0) + (1 - g_{\tau}(r)) (\ln (1 - g_{\tau}(r)) + \beta \mu_{\tau d}^0) \right]$$

$$(7)$$

where $\langle \rho_{pro,\tau}(r) \rangle$ represents the local average density of protonable τ segments of the protein, which can be calculated using

$$\langle \rho_{pro,\tau}(r) \rangle = \sum_{\theta} \int_{0}^{\infty} dr' G(r') \rho_{pro}(\theta, r') n_{\tau}(\theta, r', r)$$
 (8)

where $n_{\tau}(\theta, r', r)$ is an input quantity that gives the number τ segments that a single protein in configuration θ and center of mass of at r' places inside the spherical shell between r and r + dr. Note subscript τ denotes titratable units/residues of the protein, but this last expression also holds true for all protein segments. Namely,

$$\langle \rho_{pro,\lambda}(r) \rangle = \sum_{\theta} \int_{0}^{\infty} dr' G(r') \rho_{pro}(\theta, r') n_{\lambda}(\theta, r', r)$$
 (9)

where λ describes an arbitrary segment of the protein ($\{\tau\} \in \{\lambda\}$).

 $\mu^0_{\tau,p}$ and $\mu^0_{\tau,d}$ in Eq. (7) are the standard chemical potentials of the protonated and deprotonated τ segment respectively. In addition, $g_{\tau}(r)$ is the local degree of proton association of τ segments. If $f_{\tau}(r)$ is the local degree of charge for the segment, it follows that:

- $g_{\tau}(r) = 1 f_{\tau}(r)$ for an acid τ unit that becomes negatively charged.
- $g_{\tau}(r) = f_{\tau}(r)$ for a basic τ unit that becomes positively charged.

Next contribution to Ω_{NG} is the electrostatic energy:

$$\beta U_{elecc} = \int_{0}^{\infty} dr G(r) \left[\left(\sum_{\gamma} \rho_{\gamma}(r) q_{\gamma} + \sum_{\tau} f_{\tau}(r) \left\langle \rho_{pro,\tau}(r) \right\rangle q_{\tau} + f(r) \frac{\left\langle \phi_{MAA}(r) \right\rangle}{v_{MAA}} q_{MAA} \right) \beta \Psi(r) - \frac{1}{2} \beta \epsilon (\nabla \Psi(r))^{2} \right]$$
(10)

where $\Psi(r)$ is the position-dependent electrostatic potential, and ϵ the medium permittivity; q_{γ} is the charge of mobile species γ , q_{τ} corresponds to the charge of the titratable segments of the adsorbate, and q_{MAA} is the charge of a deprotonated MAA segment.

In this context, the average (local) electric charge density is:

$$\langle \rho_q(r) \rangle = \sum_{\gamma} \rho_{\gamma}(r) q_{\gamma} + \sum_{\tau} f_{\tau}(r) \langle \rho_{pro,\tau}(r) \rangle q_{\tau} + f(r) \frac{\langle \phi_{MAA}(r) \rangle}{v_{MAA}} q_{MAA}$$
 (11)

The next contribution to the semi-grand potential of Eq. (1) is due to the steric repulsions, which are incorporated through a physical constraint, which requires that every element of volume is fully occupied by some of the molecular species. Namely,

$$\sum_{\gamma} \rho_{\gamma}(r) v_{\gamma} + \sum_{\lambda} \left\langle \rho_{pro,\lambda}(r) \right\rangle v_{\lambda} + \sum_{i} \left\langle \phi_{i}(r) \right\rangle = 1 \qquad \forall r \tag{12}$$

where v_{λ} is the molecular volume of segment λ of the protein. Again, we emphasize that subscript λ considers all segments of the protein, including titratable (τ) and charge neutral residues. Subscript i runs over all types segments in the polymer network.

 U_{vdw} is the total energetic contribution of the van der Waals interactions. In this work, we assume that all polymer segments and protein residues have a hydrophilic character. In other words, the interactions between different pairs of segments and the segment-solvent interactions are approximately the same. As a result, the net interaction energy represents an additive constant to the total free energy.

The last contributions to the semi-grand potential of Eq. (1) incorporate the fact that the nanogel is in chemical equilibrium with a bulk solution of controlled composition. These terms include the chemical potentials of mobile species:

$$\mu_{\gamma} N_{\gamma} + \mu_{pro} N_{pro} = \int_{0}^{\infty} dr G(r) \left[\sum_{\gamma} \rho_{\gamma}(r) \mu_{\gamma} + \mu_{pro} \left\langle \rho_{pro}(r) \right\rangle + \mu_{H^{+}} \left(\sum_{\tau} g_{\tau} \left\langle \rho_{pro,\tau}(r) \right\rangle + (1 - f(r)) \frac{\left\langle \phi_{MAA}(r) \right\rangle}{v_{MAA}} \right) \right]$$
(13)

where μ_{γ} and N_{γ} are respectively the chemical potential and number of molecules of species γ . Similarly, μ_{pro} and N_{pro} are the chemical potential and the total number of proteins. The additional terms coupled to μ_{H^+} account for those protons that are bound to uncharged MAA segments and those in protonated protein residues.

Therefore, the explicit form of the semi-grand potential is

$$\begin{split} \beta\Omega_{NG} &= \sum_{\gamma} \int_{0}^{\infty} dr G(r) \rho_{\gamma}(r) \left(\ln \left(\rho_{\gamma}(r) v_{w} \right) - 1 + \beta \mu_{\gamma}^{0} \right) \\ &+ \sum_{\theta} \int_{0}^{\infty} dr G(r) \rho_{pro}(r) \left(\ln \left(\rho_{pro}(\theta, r) v_{w} \right) - 1 + \beta \mu_{pro}^{0} \right) \\ &+ \sum_{\alpha} P(\alpha) \ln P(\alpha) \\ &+ \int_{0}^{\infty} dr G(r) \frac{\langle \phi_{MAA}(r) \rangle}{v_{MAA}} \left[f(r) (\ln f(r) + \beta \mu_{MAA}^{0}) \\ &+ (1 - f(r)) (\ln (1 - f(r)) + \beta \mu_{MAAH}^{0}) \right] \\ &+ \int_{0}^{\infty} dr G(r) \sum_{\tau} \left\langle \rho_{pro,\tau}(r) \right\rangle \left[g_{\tau}(r) (\ln g_{\tau}(r) + \beta \mu_{\tau p}^{0}) \\ &+ (1 - g_{\tau}(r)) (\ln (1 - g_{\tau}(r)) + \beta \mu_{\tau d}^{0}) \right] \\ &+ \int_{0}^{\infty} dr G(r) \left[\left(\sum_{\gamma} \rho_{\gamma}(r) q_{\gamma} + \sum_{\tau} f_{\tau}(r) \left\langle \rho_{pro,\tau}(r) \right\rangle q_{\tau} \\ &+ f(r) \frac{\langle \phi_{MAA}(r) \rangle}{v_{MAA}} q_{MAA} \right) \beta \Psi(r) - \frac{1}{2} \beta \epsilon (\nabla \Psi(r))^{2} \right] \\ &+ \int_{0}^{\infty} dr G(r) \beta \Pi(r) \left(\sum_{\gamma} \rho_{\gamma}(r) v_{\gamma} + \sum_{\lambda} \left\langle \rho_{pro,\lambda}(r) \right\rangle v_{\lambda} + \sum_{i} \left\langle \phi_{i}(r) \right\rangle - 1 \right) \\ &- \int_{0}^{\infty} dr G(r) \left[\sum_{\gamma} \rho_{\gamma}(r) \beta \mu_{\gamma} + \beta \mu_{pro} \left\langle \rho_{pro}(r) \right\rangle + \beta \mu_{H} + \sum_{\tau} g_{\tau}(r) \left\langle \rho_{pro,\tau}(r) \right\rangle \\ &+ \beta \mu_{H} + (1 - f(r)) \frac{\langle \phi_{MAA}(r) \rangle}{v_{MAA}} \right] \end{split}$$

In this last expression, the Lagrange multiplier $\Pi(r)$ has been introduced to reinforce the incompresibility constraint, Eq. (12).

In Eq. (14) the thermodynamic potential has been expressed in terms of several functions:

- the local densities, $\rho_{\gamma}(r)$ and $\rho_{pro}(r)$;
- the probabilities of the different conformations of the polymer network, $P(\alpha)$;
- the electrostatic potential, $\Psi(r)$;

- the local degree of dissociation of protonable MAA segments, f(r);
- the local degrees of charge of protonable protein residues, $f_{\tau}(r)$, or alternatively their degrees of protonation, $g_{\tau}(r)$.

Minimization of $\beta\Omega_{NG}$ with respect to each of these functions yields expressions for such quantities. In particular, for the degree of charge of MAA segments in the polymer network, we calculate:

$$\frac{f(r)}{1 - f(r)} = \frac{K_{MAA}^0}{a_{H^+}} e^{-\beta \Psi(r)q_{MAA}} \tag{15}$$

Similarly, for the degree of charge of titratable units of the protein:

$$\frac{f_{\tau}(r)}{1 - f_{\tau}(r)} = \left(\frac{a_{H^{+}}}{K_{\tau}^{0}}\right)^{\mp 1} e^{-\beta \Psi(r)q_{\tau}} \tag{16}$$

where the +/- sign corresponds to a basic/acid unit. In the previous expressions, $a_{H^+}=e^{\beta\Delta\mu_{H^+}}=e^{\beta(\mu_{H^+}-\mu_{H^+}^0)}$ is the activity of protons. K^0_{MAA} and K^0_{τ} are the thermodynamic equilibrium constant of acid-base reactions of MAA and τ segments, respectively, which satisfy:

$$K_{MAA}^{0} = \exp\left(\beta \mu_{MAAH}^{0} - \beta \mu_{MAA^{-}}^{0} - \beta \mu_{H^{+}}^{0}\right)$$
 (17)

$$K_{\tau}^{0} = \exp\left(\beta \mu_{\tau p}^{0} - \beta \mu_{\tau d}^{0} - \beta \mu_{H^{+}}^{0}\right) \tag{18}$$

Optimization of Ω_{NG} with respect to the density of the small mobile species, leads to

$$\rho_{\gamma}(r)v_{w} = a_{\gamma} \exp\left(-\beta \Psi(r)q_{\gamma}\right) \exp\left(-\beta \Pi(r)v_{w}\right) \tag{19}$$

Similarly, for the density of the protein we obtain:

$$\rho_{pro}(\theta, r)v_{w} = \tilde{a}_{pro} \prod_{\tau} \exp\left[-\int_{0}^{\infty} dr' G(r') n_{\tau}(\theta, r, r') \ln f_{\tau}(r')\right]$$

$$\times \prod_{\lambda} \exp\left[-\int_{0}^{\infty} dr' G(r') n_{\lambda}(\theta, r, r') \left(\beta \psi(r') q_{\lambda} + \beta \Pi(r') v_{\lambda}\right)\right]$$
(20)

where the activity of the protein is

$$\tilde{a}_{pro} = \exp[\beta \mu_{pro} - \beta \tilde{\mu}_{pro}^0] \tag{21}$$

with:

$$\beta \tilde{\mu}_{pro}^{0} = \beta \mu_{pro}^{0} + \sum_{\tau,a} C_{n,\tau} \beta \mu_{\tau,d}^{0} + \sum_{\tau,b} C_{n,\tau} \beta (\mu_{H^{+}} - \mu_{\tau,p}^{0})$$
 (22)

 τ , a and τ , b indicate sums over acid or basic segments respectively. The composition number for a segment λ in the protein is $C_{n,\lambda}$:

$$\int_0^\infty dr' G(r') n_\lambda(\theta, r, r') = C_{n,\lambda} \quad \forall r$$
 (23)

Optimization with respect to the probability of a configuration α of the polymer network results in

$$P(\alpha) = \frac{1}{Q} \exp \left[-\sum_{i} \int_{0}^{\infty} dr G(r) \beta \Pi(r) \phi_{i}(\alpha, r) \right]$$

$$\times \exp \left[\int_{0}^{\infty} dr G(r) \ln(1 - f(r)) \frac{\phi(\alpha, r)}{v_{MAA}} \right]$$
(24)

Where *Q* is a constant that ensures $\sum_{\alpha} P(\alpha) = 1$.

The variation of Ω_{NG} with respect to the electrostatic potential results in the Poisson equation:

$$\epsilon \nabla^2 \Psi(r) = -\langle \rho_q(r) \rangle \tag{25}$$

Considering the symmetries of our problem:

$$\epsilon \frac{1}{r^2} \frac{\partial}{\partial r} \left(\frac{\partial \Psi(r)}{\partial r} \right) = -\left\langle \rho_q(r) \right\rangle \tag{26}$$

Another physical constraint to take into account at this point is the electroneutrality of the system, which is:

$$\int_0^\infty dr G(r) \left\langle \rho_q(r) \right\rangle = 0 \tag{27}$$

This constraint is satisfied by imposing the appropriate boundary condition to when solving Eq. (26). These boundary condition are:

$$\lim_{r \to \infty} \Psi(r) = 0 \tag{28}$$

$$\lim_{r \to \infty} \Psi(r) = 0 \tag{28}$$

$$\frac{d\Psi(r)}{dr} \bigg|_{r=0} = 0 \tag{29}$$

Now all of the functions that compose the thermodynamic potential Ω_{NG} have now been expressed in terms of the local electrostatic potential $\Psi(r)$, the position-dependent osmotic pressure $\Pi(r)$, and some input quantities that include the activities of the free species. Given the salt concentration, the pH and the concentration of proteins in the bulk solution, all these activities can be calculated from imposing the incompressibility and charge neutrality constraint to such solution and using the equilibrium condition of water self-dissociation. Then, the only remaining unknowns are $\Psi(r)$ and $\Pi(r)$ at each r. These local functions are calculated by numerically solving Eq. (12) and Eq. (26) at each shell r.

1.2. Bulk solution

The nanogel we study is in chemical equilibrium with a bulk solution. The chemical composition of this solution enters the theoretical framework described in the previous section through the activities of the free species. In this section, we derive expressions for those activities in terms of the chemical composition of bulk solution.

The bulk solution can be thought as taking the limit $r \to \infty$ in the expressions obtained in Section 1.1

$$\Pi^b = \Pi(r \to \infty) \tag{30}$$

$$\Psi^b = \Psi(r \to \infty) = 0 \tag{31}$$

$$\rho_{\gamma}^{b} = \rho_{\gamma}(r \to \infty) \tag{32}$$

$$\rho_{pro}^{b}(\theta) = \rho_{pro}(\theta, r \to \infty) \tag{33}$$

$$f_{\tau}^{b} = f_{\tau}(r \to \infty) \tag{34}$$

Therefore, for bulk density of free species γ we derive:

$$\rho_{\gamma}^b v_w = a_{\gamma} e^{-\beta \Pi^b v_w} \tag{35}$$

The bulk density of protein in its molecular conformation θ is:

$$\rho_{pro}^{b}(\theta)v_{w} = \tilde{a}_{pro} \prod_{\tau} \exp\left[-C_{n,\tau} \ln f_{\tau}^{b}\right]$$

$$\prod_{\lambda} \exp\left[-C_{n,\lambda}(\beta \Pi^{b} v_{\lambda} + \beta \Psi^{b} q_{\lambda})\right]$$
(36)

The total protein density in the bulk solution is

$$\left\langle \rho_{pro}^{b}\right\rangle =\sum_{\theta}\rho_{pro}^{b}(\theta)$$
 (37)

while the bulk segment density can be expressed as

$$\left\langle \rho_{pro,\lambda}^{b}\right\rangle = \left\langle \rho_{pro}^{b}\right\rangle C_{n,\lambda} \tag{38}$$

Moreover, the bulk degree of dissociation of τ segments of protein is:

$$\frac{f_{\tau}^{b}}{1 - f_{\tau}^{b}} = \left(\frac{a_{H^{+}}}{K_{\tau}^{0}}\right)^{\mp 1} \tag{39}$$

In addition, the incompressibility constraint must be applied to this bulk of the solution, which is:

$$\sum_{\gamma} \rho_{\gamma}^{b} v_{\gamma} + \sum_{\lambda} \left\langle \rho_{pro,\lambda}^{b} \right\rangle v_{\lambda} = 1 \tag{40}$$

The bulk solution must be charge-neutral,

$$\sum_{\gamma} \rho_{\gamma}^{b} q_{\gamma} + \sum_{\tau} f_{\tau}^{b} \left\langle \rho_{pro,\tau}^{b} \right\rangle q_{\tau} = 0 \tag{41}$$

The bulk densities are input quantities of each calculation. Once the pH, salt concentration and protein concentration are all set, these densities are completely determined using the incompressibility of the bath solution, Eq. (40) that provides Π^b ; electroneutrality, Eq. (41) that gives the relation between NaCl concentration, $\rho^b_{Cl^-}$ and $\rho^b_{Na^+}$; and the equilibrium constant of water self-dissociation that gives the relation between pH, $\rho^b_{OH^-}$, $\rho^b_{H^+}$.

1.3. Numerical implementation

To obtain results from the molecular theory described in the previous sections, the system of nonlinear integro-differential equations given by Eq. (12) and Eq. (26) must be solved numerically. To achieve this, the volume of the system is divided into shells of thickness $\delta = 0.5\,\mathrm{nm}$. In the expression presented in Section 1.1 sums over shells replace integrals along the r-coordinate, while finite differences substitute derivatives.

Then, the incompressibility constraint of Eq. (12) can now be expressed as:

$$\sum_{\gamma} \rho_{\gamma}(i_r) v_{\gamma} + \sum_{\lambda} \left\langle \rho_{pro,\lambda}(i_r) \right\rangle v_{\lambda} + \sum_{i} \left\langle \phi_i(i_r) \right\rangle = 1 \tag{42}$$

which gives an equation for each shell i_r , whose position is described by the coordinate $r_i = (i_r - 0.5)\delta$. The integer i_r takes values from 1 to n_r , where n_r is sufficiently large such that all densities of the free species as well as the electrostatic potential smoothly converge to the bulk solution values. Namely, $\Pi(n_r) \approx \Pi^b$, $\Psi(n_r) \approx 0$, $\rho_{\gamma}(n_r) \approx \rho_{\gamma}^b$, and $\rho_{pro}(\theta, n_r) \approx \rho_{pro}^b(\theta)$, etc.

With these considerations it is possible to rewrite the equations of the Section 1.1 in the following way. Equations (15) and (16) become:

$$\frac{f(i_r)}{1 - f(i_r)} = \frac{K_{MAA}^0}{a_{H^+}} e^{-\beta \Psi(i_r) q_{MAA}}$$
(43)

$$\frac{f_{\tau}(i_r)}{1 - f_{\tau}(i_r)} = \left(\frac{a_{H^+}}{K_{\tau}^0}\right)^{\mp 1} e^{-\beta \Psi(i_r)q_{\tau}} = \frac{f_{\tau}^b}{1 - f_{\tau}^b} e^{-\beta \Psi(i_r)q_{\tau}} \tag{44}$$

For the discretized version of Eq. (19) that gives the local density of small free species is

$$\rho_{\gamma}(i_r)v_w = a_{\gamma} \exp\left(-\beta \Psi(i_r)q_{\gamma}\right) \exp\left(-\beta \Pi(i_r)v_w\right) \tag{45}$$

while for the local protein density, Eq. (20) becomes

$$\rho_{pro}(\theta, i_r) v_w = \tilde{a}_{pro} \prod_{\tau} \exp \left[-\delta \sum_{j_r=1}^{n_r} G(j_r) n_{\tau}(\theta, i_r, j_r) \ln f_{\tau}(j_r) \right]$$

$$\times \prod_{\lambda} \exp \left[-\delta \sum_{j_r=1}^{n_r} G(j_r) n_{\lambda}(\theta, i_r, j_r) \left(\beta \Pi(j_r) v_{\lambda} + \beta \Psi(j_r) q_{\lambda} \right) \right]$$

$$(46)$$

The probability of a conformation $\{\alpha\}$ of the polymer network, 24, is also discretized to:

$$P(\alpha) = \frac{1}{Q} \exp \left[-\delta \sum_{i} \sum_{i_{r}=1}^{n_{r}} G(i_{r}) \beta \Pi(i_{r}) \phi_{i}(\alpha, i_{r}) \right]$$

$$\exp \left[\delta \sum_{i_{r}=1}^{n_{r}} G(i_{r}) \ln(1 - f(i_{r})) \frac{\phi(\alpha, i_{r})}{v_{MAA}} \right]$$
(47)

Finally the Poisson equation: \cref{} ... 26

$$\epsilon \frac{\Psi(i_r+1) - 2\Psi(i_r) + \Psi(i_r-1)}{\delta^2} + 2\epsilon \frac{\Psi(i_r+1) - \Psi(i_r)}{(i_r-0.5)\delta^2} = -\langle \rho_q(i_r) \rangle$$
(48)

where the discrete local charge density is: \cref{} ...11

$$\langle \rho_q(i_r) \rangle = \sum_{\gamma} \rho_{\gamma}(i_r) q_{\gamma} + \sum_{\tau} f_{\tau}(i_r) \langle \rho_{pro,\tau}(i_r) \rangle q_{\tau} + f(i_r) \frac{\langle \phi_{MAA}(i_r) \rangle}{v_{MAA}} q_{MAA}$$
 (49)

And the the boundary condition is: \cref{} ... 29

$$\frac{\Psi(1) - \Psi(0)}{\delta} = 0 \tag{50}$$

In general, given the pH bulk solution, salt concentration, and protein concentration,

the unknowns remaining are $\Pi(i_r)$ and $\Psi(i_r)$ for each shell i_r . These quantities can be obtained solving the system of nonlinear coupled equations given by Eqs. (42) and (48). The number of equations to be solved (and that of unknowns) is $2n_r$ the total number of shells. The number of terms in each equation is roughly of the same order of magnitude as the total number of molecular conformations (network and protein) included in the calculation. These equations are solved numerically using a Jacobian-Free Newton method.