MAFI Lab.

Dept. of Information and communication Engineering, DGIST





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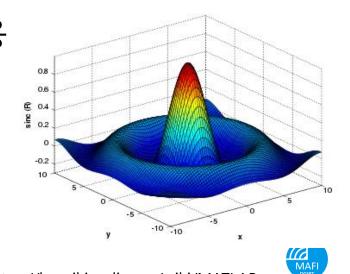
- Motivation
- Installation
- MATLAB Basic
 - 행렬 연산
 - 제어 흐름
 - √ for
 - √ if/elseif/else
 - 그래프 작성
 - ✓ plot
 - ✓ stem
 - ✓ subplot





Motivation

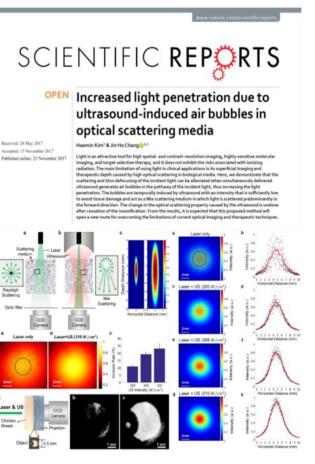
- MATLAB (MATrix + LABoratory)
 - MathWorks 사에서 개발한 수치 해석 및 프로그래밍 환경을 제공하는 공학용소프트웨어
 - 행렬을 기반으로 한 계산 기능을 지원하며, 함수나 데이터를 그림으로 그리는 기능 및 프로그래밍을 통한 알고리즘 구현 등을 제공
 - 수치 계산이 필요한 과학 및 공학 분야에서 다양하게 사용





Motivation

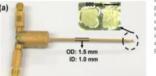
• MATLAB의 활용

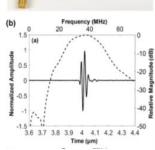


Dual-Element Intravascular Ultrasound
Transducer for Tissue Harmonic Imaging and
Frequency Compounding: Development and
Imaging Performance Assessment

Junsu Lee , Student Member, IEEE, and Jin Ho Chang , Senior Member, IEEE

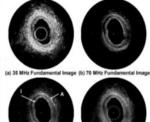
Abstract—Objective: For accurate diagnosis of atteroscierosis, the high spatial and contrast resolutions of intravascular ultrasound (iVUS) images are a key requirement. Increasing the center frequency of IVUS is a simple solution to meet this requirement. However, this leads to a reduction in imaging depth due to the frequency-dependent attenuation of ultrasound. Here, we report a recently developed dual-element IVUS transducer for tissue harmonic imaging (THI) and frequency compounding to increase the spatial and contrast resolutions of IVUS images, while imaging (THI) and frequency compounding to increase the spatial and contrast resolutions of IVUS images, while imaging the imaging of the spatial and segment in the spatial and seen the spatial and special contrast resolutions of IVUS images, while imaging the imaging of the spatial properties of the spatial contrast resolutions of IVUS images, while images and the other 70-MHz element is used for producing general IVUS images and the other 70-MHz element is or receiving the second harmonic signals induced by the 35-MHz ultrasound. The fundamental and second harmonic signals can also be used for frequency compound imaging to further improve contrast





1. Імпероистом

THEROSCLEROSIS is a typical arterial disease, in which A plaques build up in artery walls, and the leading cause of leath and disability [1]. To determine the direction of treatment, it is clinically important to identify vulnerable plaque as well as to measure the atherosclerotic plaque burden and the degree of luminal stenosis. Vulnerable plaque is typically characterized by a large lipid core shielded by a thin fibrous cap ($<65 \mu m$) [2]. The measurement of atherosclerotic plaque burden and luminal stenosis requires clear visualization of the plaque, the lumen, and the blood vessel layers [1], [3]. Although angio graph, computed tomography (CT), and magnetic resonance imaging (MRI) can be used for diagnosis of atherosclerosis as noninvasive imaging tools, intravascular ultrasound (IVUS) imaging has a very high potential for accurately assessing the plaque vulnerability, atherosclerotic plaque burden, and luminal stenosis [4]-[6]. In addition, this imaging modality can be used for the real-time guidance of percutaneous coronary intervention (PCI) [6]. To minimize the complications of stent implantation, especially, the information about incomplete stent apposition, stent underexpansion, and edge dissection should be provided by IVUS images [7]. Due to low spatial and contrast



Nanoscale

PAPER

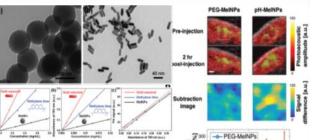


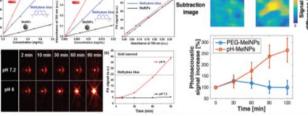
pH-Induced aggregated melanin nanoparticles for photoacoustic signal amplification†

Kuk-Youn Ju.‡^a Jeeun Kang.‡^b Jung Pyo.^a Joohyun Lim.^a Jin Ho Chang^{ab} and Jin-Kyu Lee^a

We present a new melann-like nanopartice (MeNP) and its performance evaluation results. This particle is proposed as an exogenous contrast agent for photoacoustic (PAI imaging. Conventional PAI contrast agents are based on non-tiological insterials. In contrast, the MeNPs are organic nanoparticles inspired by natural motions. Mainrin is an endispenous chromophore that has the ability to produce a PA signal in vivo. The developed MeNPs are capable of algorithmic produce and produce of the signal in vivo. The developed MeNPs are capable of algorithmic annies on the surface of base MeNPs. We ascentained that the physical aggregation of the MeNPs resulted in an increased PAI signal strength in the near-infrared window of biological strase (i.e., 700 nm) without absorption furning. This phenomenon is likely because of the overlapping thermal fields of the developed MeNPs. The PAI signal produced from the developed MeNPs, the response to mindly succisc conditions. Exp. pH 6.1 is \$1 increas stonger than under neutral conditions. This unique chreateristic found in this study can be utilized in a practical strategy for highly sensitive on vivo cancer target imaging in response to this acidic microenvieroment. This approach to amplify the PAI response of the MeNPs in inclusers could accelerate the use of MeNPs in an alternative to non-belogical nanoprobles, so that MeNPs may be applicable in PAI imaging and functional PAI imaging such as stemplic sensitive.









polis accorp/pornel/april

Resonance-Based Frequency-Selective Amplification for Increased Photoacoustic Imaging Sensitivity

Haemin Kim, ** Hohyeon Lee, *** Hyungwon Moon, ** Jeeun Kang, *** Yongho Jang, ** Doyeon Kim, ** Jinwoo Kim, ** Elizabeth Huynh, ** Lang Zheng, ** Hyuncheol Kim, *** ** and Jin Ho Chang. *** ** Tang Zheng, ** Hyuncheol Kim, *** ** Tang Zheng, *** ** Tang Zheng, *** Tang

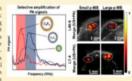
Department of Biomedical Engineering, ¹Department of Chemical and Biomelecular Engineering, and ⁸Department of Electroni Engineering, Sogang University, 35 Backboom-ro, Mapo-gu, Seoul 04107, South Korea

^{II}Ontario Cancer Institute, University Health Network, Toronto, Ontario M5G1L7, Canada

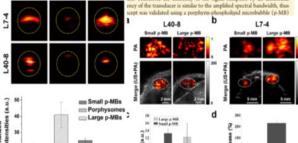
¹Department of Medical Biophysics, University of Toronto, Toronto, Ontario MSG11.7, Canada

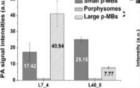
O Supporting Information

ABSTRACT: Photoacoustic (PA) imaging has attracted much attention as a new biomedical imaging modality due to its ultrasonic spatial resolution, optical context resolution, and deeper imaging depth than other optical imaging modalities. Eugenous PA contrast agents have been developed, with high optical absorbance at a desired wavelength, to improve their imaging sensitivity over background signal produced from endogenous nonangited absorbance. As monoptimal detection of PA isgual, due to the fast that the PA signal contains a broad stage of frequency components, whereas an ultrasound transducers is only capable of receiving signals within a figulae within a speak of the pages of the page of th



certain frequency range. As a result, much of the signal generated by PA contrast agont is lost when received by an ultrasound ramsduccr. In this study, we propose a new concept for PA contrast enhancement. This method uses chromophore embedded Small p-MBs Porphysomes Large p-MBs we could be PA signal energy stithin a desired spectral bandwidth can be size. Therefore, the efficiency of the signal reception by an ultrasound











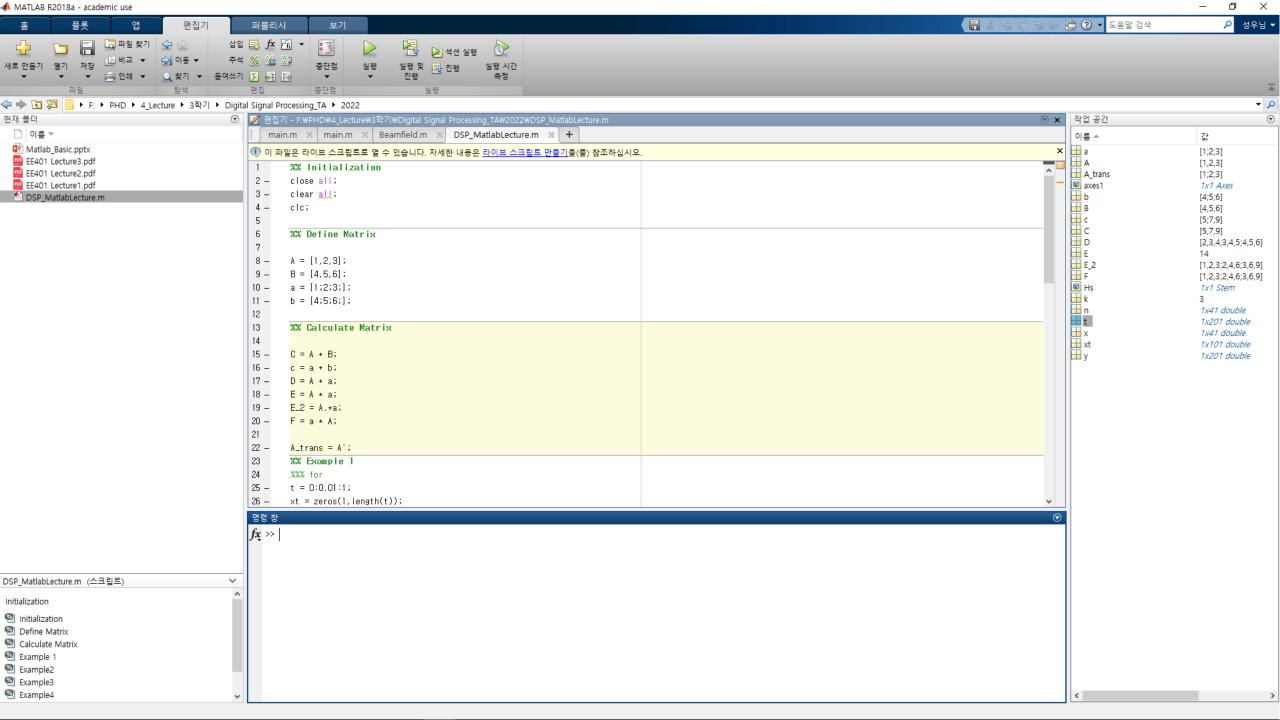
Installation











MATLAB

– 연산자(operator)

부호	이름	부호	이름
=	대입	==	동등
+	덧셈	-	뺄셈
*	곱셈	.*	배열 곱셈
٨	거듭제곱	.^	배열 거듭제곱
/	나눗셈	./	배열 나눗셈
<>	관계 연산자	&	논리 AND
	논리 OR	~	논리 NOT
1	전치		배열 전치



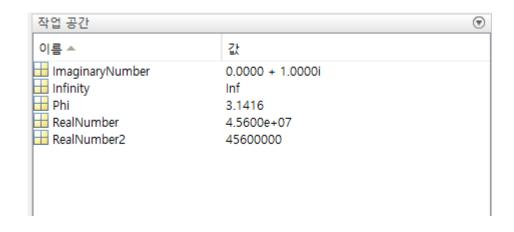


MATLAB

- 수(number)

```
✓ Ex) 실수 4.56x10^7 => 4.56e7, \sqrt{-1} => 1i, \pi => pi, \infty => inf
```

```
| Z 편집기 - F:\PHD\4_Lecture\3학기\Digital Signal Processing_TA\2022\DSP_MatlabLecture.m
    DSP_MatlabLecture.m × +
         XX Initialization
         close all;
         clear all;
         cle;
         RealNumber = 4.56*10^7;
         RealNumber2 = 4.56e7;
  8
  9 -
         ImaginaryNumber = sqrt(-1);
 10
 11 -
         Phi = pi;
 12
 13 -
         Infinity = inf;
```







MATLAB

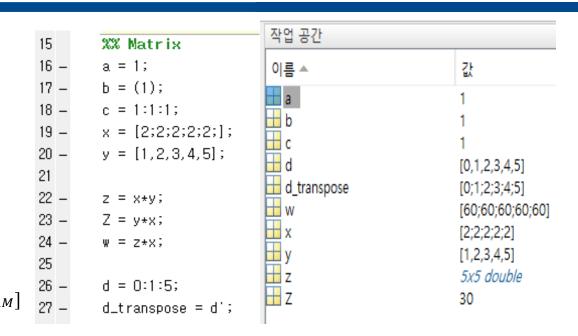
- 변수(variable)
 - ✔1. 행렬(matrix)
 - ✓ 2. 배열(array)
 - 스칼라(scalar)
 - 열 벡터(column vector)

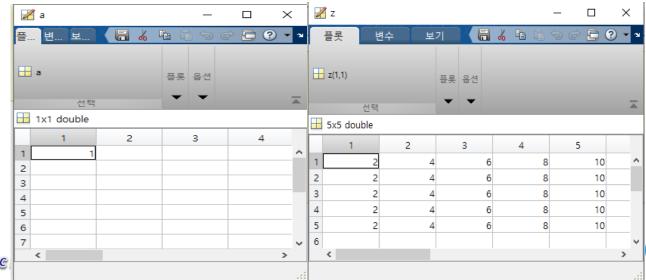
$$Y = [y_{1j}]_{j:1,...,M} = [y_{11} \quad \cdots \quad y_{1M}]$$

• 행 벡터(row vector)

ow vector)
$$X = [x_{i1}]_{i:1,...,N} = \begin{bmatrix} x_{11} \\ \vdots \\ x_{N1} \end{bmatrix}$$

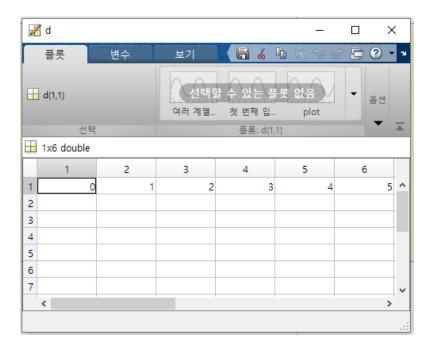
• 일반 행렬



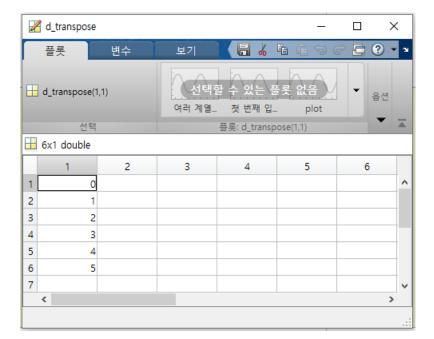




- 행렬 연산
 - 전치(transposition)
 - ✓ 모든 행(열)이 열(행)로 바뀌는 연산
 - ✓ Ex). d가 (1 x 6)행렬이라고 할 때, d' = [d_{ji}]; j = 1,...6, i = 1











- 행렬 연산
 - 벡터-벡터 곱셈
 - Ex). x를 (N x 1), y를 (1 x M) 벡터 일 때,

$$x * y => xy = \begin{bmatrix} x_1 \\ \vdots \\ x_N \end{bmatrix} [y_1 \quad \cdots \quad y_M] = \begin{bmatrix} x_1 y_1 & \cdots & x_1 y_M \\ \vdots & \ddots & \vdots \\ x_N y_1 & \cdots & x_N y_M \end{bmatrix}$$

- 만약 M = N이라면,

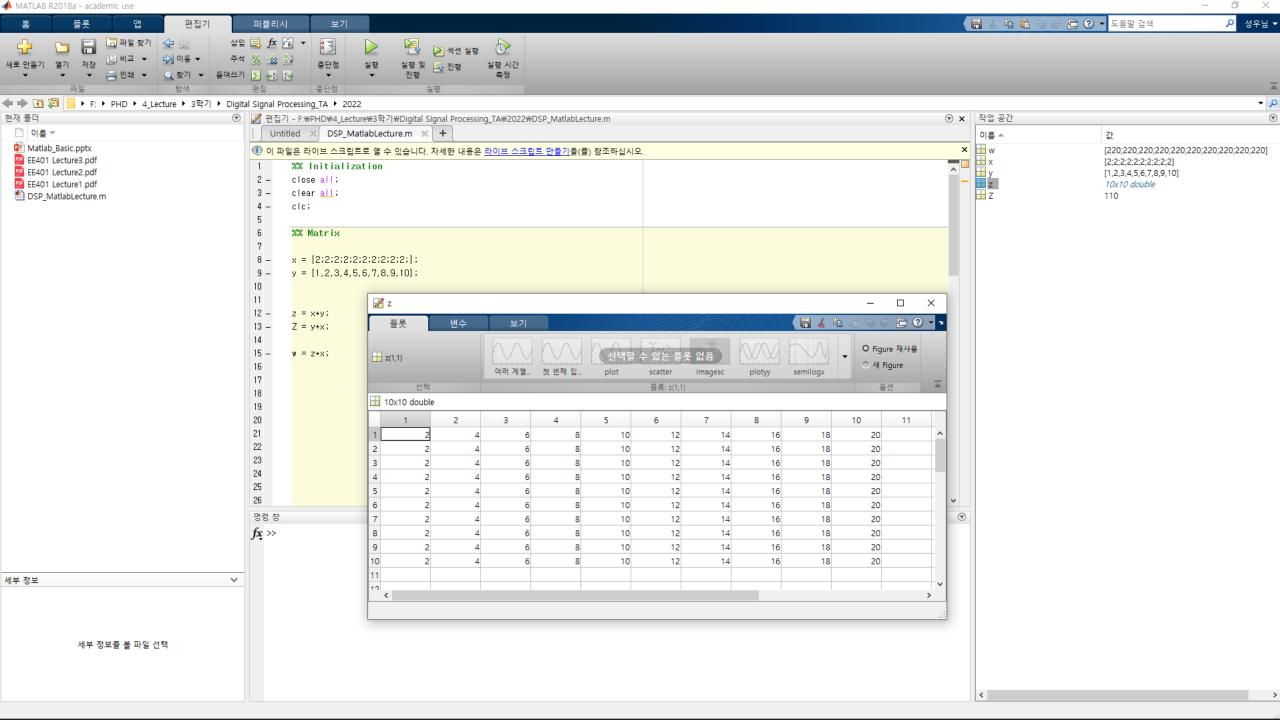
$$y * x => yx = [y_1 \quad \cdots \quad y_N] \begin{bmatrix} x_1 \\ \vdots \\ x_N \end{bmatrix} = x_1y_1 + \dots + x_Ny_M$$

- 행렬-벡터 곱셈

$$y = A * x => Ax = \begin{bmatrix} a_{11} & \cdots & a_{1M} \\ \vdots & \ddots & \vdots \\ a_{N1} & \cdots & a_{NM} \end{bmatrix} \begin{bmatrix} x_1 \\ \vdots \\ x_M \end{bmatrix} = \begin{bmatrix} y_1 \\ \vdots \\ y_N \end{bmatrix}$$







- 제어 흐름
 - for loop
 - ✓ 지정된 횟수를 반복하는 for루프

- 예제

$$x(t) = \sin(2\pi t) + \frac{1}{3}\sin(6\pi t) + \frac{1}{5}\sin(10\pi t) = \sum_{k=1}^{3} \frac{1}{k}\sin(2\pi kt), 0 \le t \le 1$$





- 제어 흐름
 - if/elseif/else
 - ✓ 조건이 true인 경우 명령문 실행

```
if condition1
command1
elseif condition2
command2
else
command3
end
```

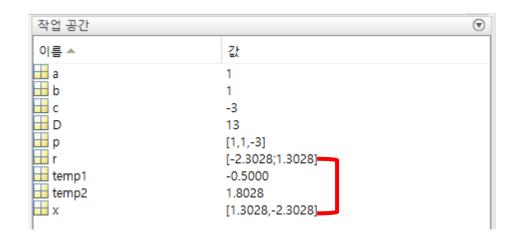




• 제어 흐름

$$-$$
 if/elseif/else 예제 $ax^2 + bx + c = 0$ 의 근, $x = \frac{-b \pm \sqrt{b^2 - 4ac}}{2a}$

```
XX
       a = 1;
       b = 1;
       c = -3;
       D = b^2-4*a*c;
12 -
       temp1 = -b/(2*a);
13
14 -
       if (D == 0)
15 -
        x = temp1;
       elseif (D > 0)
        temp2 = sqrt(D)/(2*a);
18 -
       x(1) = temp1+temp2;
19 -
           x(2) = temp1-temp2;
20 -
       else
21 -
           sprintf('Not Exist');
22 -
       end
       %%% Matlab function
       p = [a, b, c];
       r = roots(p);
```



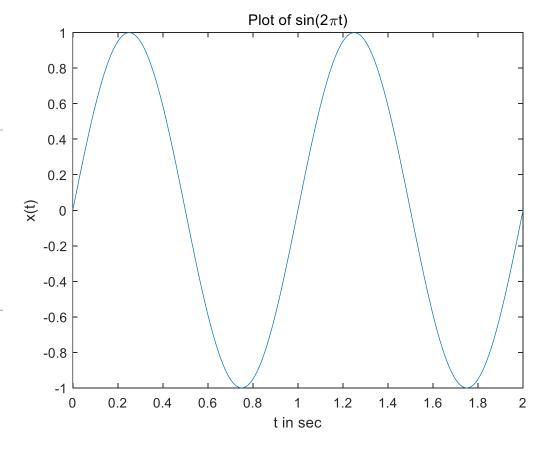




• 그래프 작성

- plot(t,x)

```
59
        XX Example2
60
        %%% plot
        t = 0:0.01:2;
                                        %%% sample points from O to 2 in steps of 0.01
62 -
       x = sin(2*pi*t);
                                        %%% Evaluate sin(2 pi t)
63
64 -
        plot(t,x);
                                        %%% create plot with blue line
       xlabel('t in sec');
                                        %%% Label x axis
       ylabel('x(t)');
                                        %%% Label y axis
        title('Plot of sin(2\pit)');
                                        %%% Title Plot
```



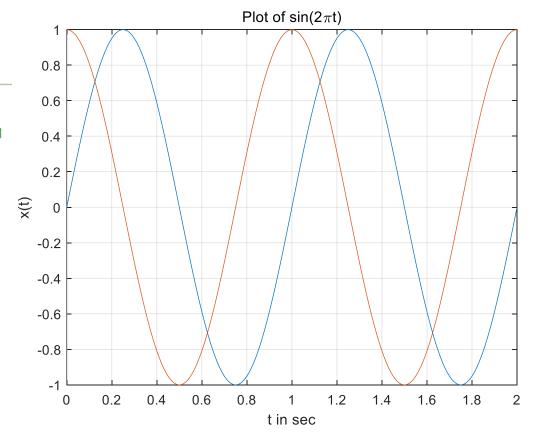




• 그래프 작성

- plot(t,x)

```
63
        XX Example2
64
        %%% plot
65 -
        t = 0:0.01:2;
                                        %%% sample points from O to 2 in steps of 0.01
66 -
        x = sin(2*pi*t);
                                        %%% Evaluate sin(2 pi t)
67 -
        y = cos(2*pi*t);
68
69 -
        plot(t,x);
                                        %%% create plot with blue line
70 -
        hold on;
71 -
        grid on;
        plot(t,y);
73 -
        xlabel('t in sec');
                                     %%% Label x axis
74 -
        ylabel('x(t)');
                                      %%% Label y axis
        title('Plot of sin(2\piit)'); %%% Title Plot
75 -
```

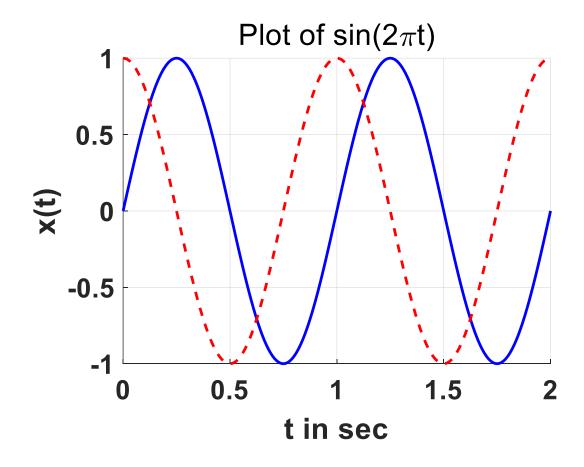






• 그래프 작성

- plot(t,x)



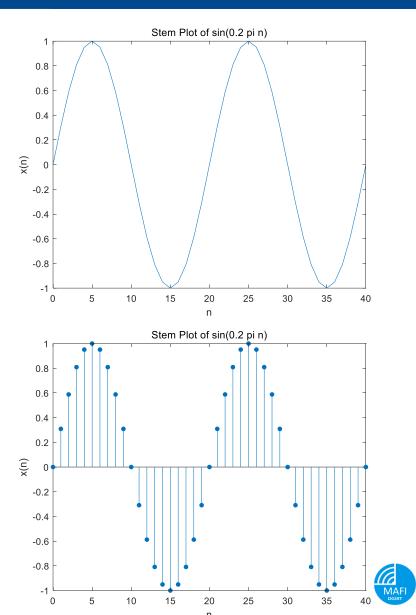




• 그래프 작성

- stem

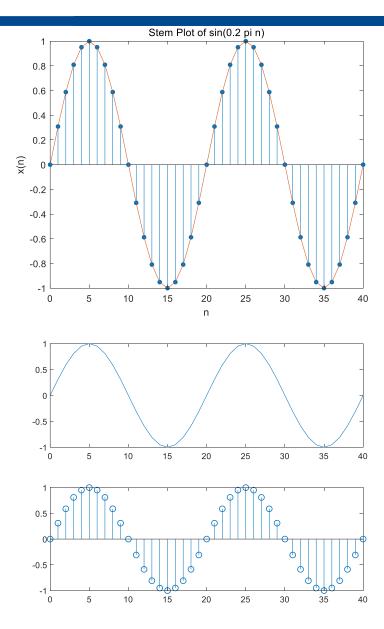
```
55
      XX Example4
      %%% stem
      n = 0:1:40;
                                    %%% sample index from 0 to 20
      x = sin(-.1*pi*n);
                                    - %%% Evaluate sin(0,2 pi n)
59 -
      60 -
      set(Hs,'markersize',4);
                                    XXX Change circle size
61 -
      xlabel('n');
                                    %%% Label x axis
62 -
      ylabel('x(n)');
                                    %%% Label y axis
63 -
      title('Stem Plot of sin(0,2 pi n)'); %%% Title plot
```





• 그래프 작성

subplot







Thank you

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