Volatile Organic Compound Detection Using Insect Odorant-Receptor Functionalised Field-Effect Transistors

by

Eddyn Oswald Perkins Treacher

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Te Herenga Waka - Victoria University of Wellington

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Acknowledgements

Thanks for all the fish.

Abstract

This is a thesis skeleton written with quarto. Make a copy of this thesis repo and start to write!

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1. Introduction

This is a book created from markdown and executable code.

See for additional discussion of literate programming.

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2. Carbon Nanotube and Graphene Field-Effect Transistors

2.1. Device Functionalisation

2.2. Insect Odorant Receptors

3. Carbon Nanotube and Graphene Field-Effect Transistors as Biosensor Platforms

4. Fabrication of Carbon Nanotube Network and Graphene Field-Effect Transistors

This chapter discusses the fabrication processes for both the carbon nanotube network and graphene transistors. Experimental optimisation of the transducer element is critical for biosensor work, and large numbers of transducers were required for testing various biosensor functionalisation processes. Therefore, these processes were developed to rapidly fabricate devices with reproducible device characteristics appropriate for biosensing work. Also outlined in this chapter are the characterisation techniques taken to test the quality and reproducibility of these fabrication processes.

The nitrogen ($\geq$ 99.99%) and oxygen (99.7%) used in fabrication work was supplied by BOC Limited New Zealand. Deionised (DI) water was taken from a Synergy® UV Water Purification System. The DI water had a measured conductivity of (1.4 ± 0.1) μS cm^{-1}, compared to tap water with a measured conductivity of (7.8 ± 0.2) μS cm^{-1}.

4.1. Deposition of Carbon Nanotubes

4-inch *p*-type (B-doped) silicon wafers with either a 100 nm or 300 nm SiO_2 layer (WaferPro LLC) were used as the substrate for carbon nanotube network deposition. A 100 nm SiO_2 layer was the preferred option for the devices intended for backgated measurements.

4.1.1. Solvent-Based

The solvent-based deposition process for the carbon nanotube network in the second fabrication protocol is as follows. 5 μg of carbon nanotube bucky paper (NanoIntegris, IsoNanotubes S-99) was dispersed in 10 mL of dichlorobenzene (Sigma Aldrich) by ultrasonication until no particles were visible to the naked eye. The ultrasonic bath temperature was kept constant at 25°C. A 10 mg solution of 2-mercaptopyridine (99%, Sigma-Aldrich) was dissolved in 1 ml ethanol and drop-cast over the cleaned SiO_2/Si surface for 20 minutes, followed by rinsing in ethanol to remove residual 2-mercaptopyridine

and drying with nitrogen. The substrates were then submerged into the CNT-DCB suspension for 2 hours, dipped into ethanol for 10 min to remove excess solvent and any unattached carbon nanotube bundles, and then dried with nitrogen.

4.1.2. Surfactant-Based

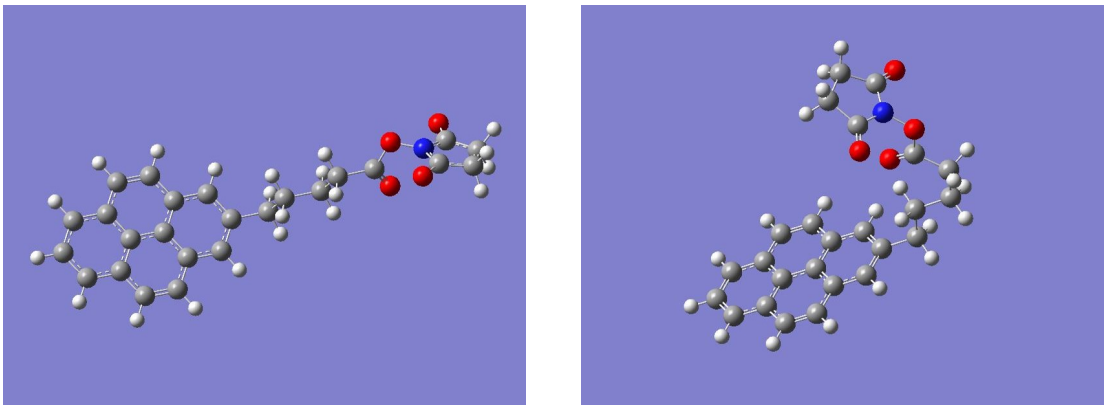
Simple Dropcasting

Steam-assisted Method

5. Functionalisation of Carbon Nanotubes and Graphene with Odorant Receptors

5.1. Linker molecules

5.1.1. 1-Pyrenebutanoic acid N-hydroxysuccinimide ester (PBASE)



(a) Hartree-Fock energy: -3427728.67 kJ/mol (9 s.f.)

(b) Hartree-Fock energy: -3427729.66 kJ/mol (9 s.f.)

Figure 5.1.: Two conformations of PBASE molecule with geometry optimised via *ab initio* calculation (computed using Gaussian 16 [1]). The difference between computed Hartree-Fock energies is 1.0 kJ/mol, small enough that the existence of both molecular conformations is physically possible.

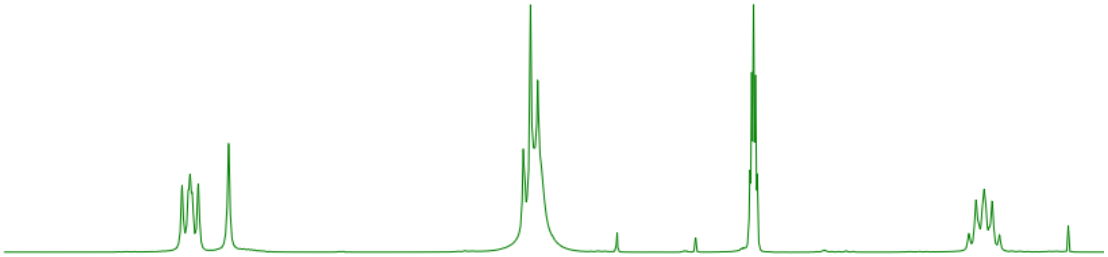
1-Pyrenebutanoic acid N-hydroxysuccinimide ester (variously known commercially and in the literature as 1-Pyrenebutyric acid N-hydroxysuccinimide ester, PBASE, PBSE, PASE, Pyr-NHS, PyBASE, PANHS) is a aromatic, bifunctional molecule commonly used for tethering biomolecules to the carbon rings of graphene and carbon nanotubes. The optimised molecular structure of PBASE is shown in Figure 5.1.

The non-covalent functionalisation of proteins onto a single-walled carbon nanotube using PBASE was first reported by Chen *et al.* in 2001 [2]. Two methods for protein functionalisation and immobilisation were successfully used, with the only differences being the solvent used to dissolve the PBASE powder (DMF, methanol) and the final

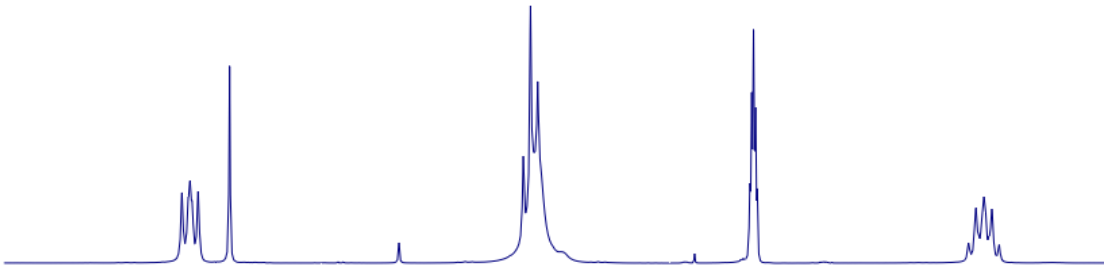
concentration of the resulting solutions (6 mM, 1 mM respectively). The lower concentration may have been used for PBASE in methanol as PBASE powder appears to dissolve poorly in methanol at higher concentrations. Cella *et al.*, Campos *et al.*, Zheng *et al.* and Ohno *et al.* all directly cite Chen *et al.* when discussing functionalisation with PBASE [3]–[6]. Other groups using PBASE for graphene or carbon nanotube functionalisation do not explicitly reference Chen *et al.* in their methodology, but it is apparent they often draw on one of these two original methods. This common ancestry becomes apparent from the high frequency of methods detailing the use of 6 mM PBASE in DMF and 1 mM PBASE in methanol, as seen in Table 5.1.

However, despite this shared heritage, it is also apparent from Table 5.1 that there is a large degree of variation in the methods used for PBASE functionalisation. Various electrical characterisation, microscopy and spectroscopy techniques have been used to demonstrate successful functionalisation. However, there has historically been little justification provided for the exact parameters used in the procedure. As noted by Zhen *et al.* and Hinnemo *et al.*, there is more generally a lack of systematic research into formation of pyrene-derivative monolayers on graphene and other carbon nanomaterials, despite the wide use of this chemistry in the literature [7], [8].

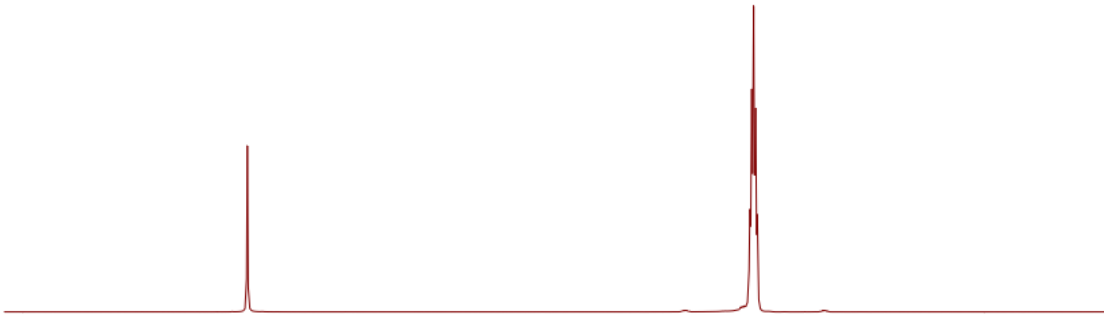
We purchased PBASE from two suppliers, Sigma-Aldrich and Setareh Biotech. Sigma recommends DMF and methanol as suitable solvents for dissolving PBASE alongside chloroform and DMSO. Setareh Biotech indicates methanol can be used for dissolving PBASE. The two suppliers have conflicting information for suitable storage of PBASE, with Sigma recommending room temperature storage while Setareh Biotech recommends storage of -5 to -30°C and protection from light and moisture. Figure 5.2 compares the shapes of NMR spectra of PBASE from each supplier dissolved in DMSO, alongside a blank DMSO spectrum.



(a) Sigma PBASE in DMSO



(b) Setareh PBASE in DMSO



(c) Blank (DMSO only)

Figure 5.2.: Comparison of NMR spectrum profiles (arbitrary units)

Table 5.1.: Comparison of PBASE functionalisation processes used for immobilisation of proteins and aptamers onto liquid-gated CNTFET and graphene FET sensors

Solvent	Channel	Conc. (mM)	Incubation type	Time (hr)	Rinse steps	References
DMF	CNTs	5	Immersed	1	PBS	Maehashi *et al.* [9]
		6	Immersed	1	DMF, PBS	García-Aljaro *et al.* [10]
		6	Immersed	1	DMF	Chen *et al.* [2]
		6	Immersed	1	DMF	Cella *et al.* [3]
		6	Immersed	1	DMF	Das *et al.* [11]
	Graphene	-	-	2	DMF	Kwong Hong Tsang *et al.* [12]
		-	-	20	-	Wiedman *et al.* [13]
		0.2	Immersed	20	DMF, IPA, DI water	Gao *et al.* [14]
		1	100 μL droplet	6	DMF, IPA, DI water	Nekrasov *et al.* [15]
		5	Immersed	1	DMF, DI water	Hwang *et al.* [16]
		6	6 μL droplet	2	DMF, DI water	Nur Nasufiya *et al.* [17]
		10	10 μL droplet	2	DMF, DI water	Campos *et al.* [4]
		10	Immersed	2	DMF, PBS	Kuscu *et al.* [18]
		10	Immersed	1	DMF	Xu *et al.* [19]
		10	Immersed	12	DMF, ethanol, DI water	Khan *et al.* [20]
2-Methoxyethanol	Graphene	1	Immersed	1	DI water	Ono *et al.* [21]
Methanol	CNTs	1	Immersed	1	Methanol, DI water	Zheng *et al.* [5]
		1	Immersed	2	Methanol	Kim *et al.* [22]
	Graphene	5	Immersed	2	-	Sethi *et al.* [23]
		5	Immersed	1	Methanol, PBS	Ohno *et al.* [6]
DMSO	CNTs	10	-	1	DI water	Lopez *et al.* [24]
		10	Immersed	1	PBS	Strack *et al.* [25]

6. Results

What I found out.

See for more detailed results

7. Vapour Phase Sensing with Transistor Biosensors

7.1. Testing Vapour Delivery System

7.1.1. System Description

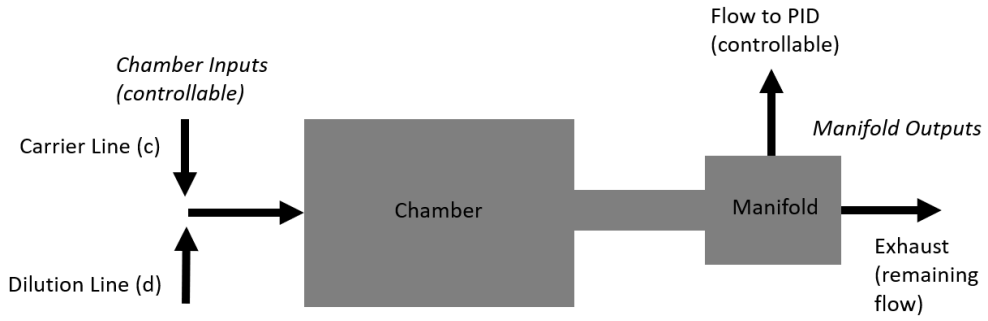


Figure 7.1.: Vapour Delivery System - Schematic of device chamber and manifold

7.1.2. Temperature and Humidity Indicator

7.1.3. Photoionisation Detector

Bubbling Vapour

First year report: “ ““First, a 200 sccm flow of N2 gas was sent through the dilution line to the device chamber until 1000 s. Then, the flow controller three-way valves were manually adjusted so that the same 200 sccm flow was directed through 50 mL of EtOH analyte in the carrier line. This continued until 2200 s, where the valves were again manually adjusted so that 200 sccm clean N2 again flowed through the device chamber. The resulting current across the device channel was monitored over this time, and is shown in Figure 19. A response to EtOH exposure and removal is visible.”“ ”

8. Summary

In summary, this book has no content whatsoever.

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A. Photolithography

This section details some of the standard photolithography procedures used in the device fabrication processes detailed in Chapter 4. Photoresists, also referred to here as "resists", are UV light-sensitive polymeric resins used for photolithography. Photolithography procedures should be performed under yellow lighting, as light wavelengths from 320-450 nm can promote photo reactions in the photoresist used. Aging of photoresist over time can also significantly affect the photolithography process, and therefore all processes should be re-optimised regularly over time to give the desired result [26]. The range in processing times for some steps of the processes used here are largely due to the effects of aging on the photoresist.

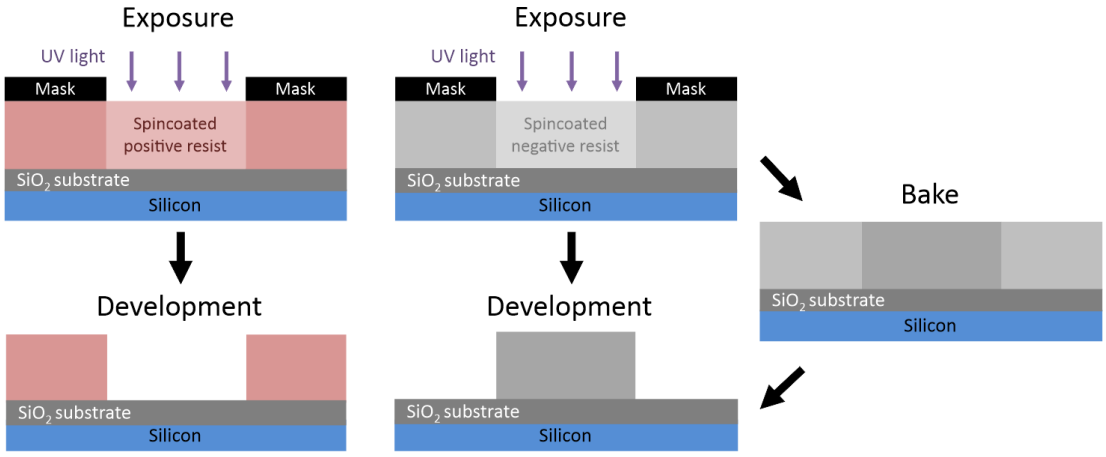
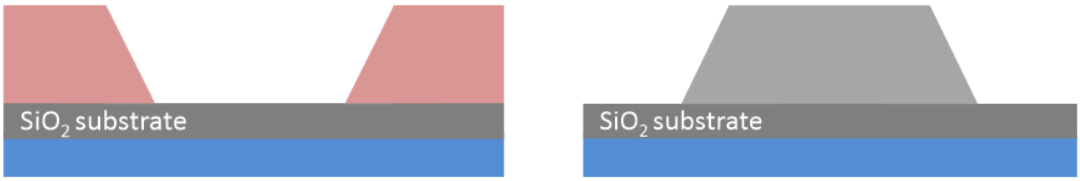


Figure A.1.: A side-view comparison of generic photolithography processes for positive and negative resists in the ideal case. Photolithography with a positive resist requires a single softbake step before exposure, while for negative resists a second baking step is required after exposure (Thicknesses shown not to scale).

Photolithography was performed using both positive and negative photoresists. Positive resists are made soluble in alkalines by UV light exposure, meaning exposed areas are removed in the development process. Conversely, negative resists are cross-linked by exposure and a post-exposure bake step. All photolithographic exposure was performed on a Karl Suss MJB3 Contact Aligner with a USHIO SHP 350 W lamp (USH-350DS, Japan). When performing lithography, the intensity reading from the aligner was 20.8 - 22.6 mW/cm^2 (Note however that an external photometer reading at 400 nm found an

intensity output of 17.2 mW/cm^2 when the aligner read 21.0 mW/cm^2). The unexposed areas of the negative resist are then removed in the development process [26]. Figure A.1 gives a visual representation of these differences.



(a) Overcut profile of a positive resist (b) Undercut profile of a negative resist

Figure A.2.: Two different resist profiles seen for different types of photoresist. The undercut profile is ideal for thin-film metal deposition and subsequent patterned removal, known as "lift-off".

The specific photoresist selected for photolithography depends on the specific use case. The types used in this thesis are positive and negative AZ® photoresists (AZ® 1518, Microchem, Germany; AZ® nLOF 2020, Microchem, Germany) and solid SU-8 (GM 1060, Gersteltec, Switzerland). The AZ® resists used here have a minimum film thickness of 1.5 μm [26], while the GM 1060 SU-8 has a minimum film thickness of 5 μm [27]. Positive resists which have not been thermally crosslinked will soften at higher temperatures ($\gtrsim$ 100°C for AZ® 1518), leading to a rounded profile. This is not the case for negative resists, which are more thermally stable [26]. Each resist therefore has a different cross-section profile, as shown in Figure A.2.

The negative resist profile is more suited to metal or metal oxide deposition and lift-off processes [26], though the process is more sensitive to error due to the extrarequiring more processing steps than positive resist. Finally, when it is suitably processed SU-8 is considered to be more biocompatible than other photoresists. It is especially biocompatible when chemically modified via processes such as isopropanol sonication and O_2 plasma treatment [28].

The step-by-step processes for each resist are detailed here in the subsequent sections.

A.1. AZ® 1518 photoresist

1. Spincoat at 4000 rotations per minute (rpm) for 1 minute (note: use the minimum amount of photoresist required to fully cover the wafer surface)
2. Softbake 2-4 minutes at 95°C on the hotplate (2 min for individual devices, 4 min for a quarter wafer)
3. Mask expose for 10-12 s (note: clean mask with acetone/IPA and N_2 dry before use)

4. Develop with 3 parts AZ® 326 (2.38 % TMAH metal-ion free developer, Microchem, Germany) in 1 part deionised (DI) water for 30-45 s (note: rinse for 10-15 s in one development solution, then perform the rest of the development in clean developer for a cleaner profile)

B. Python Code for Data Analysis

C. Vapour Delivery System

C.1. Technical Notes

Two LabView Virtual Instruments (VIs) were adapted from pre-existing VIs for operating the mass flow controllers and monitoring vapour flow into the device chamber, as well as monitoring temperature and humidity in the vapour delivery system's manifold. These VIs were named " " A third VI was developed in parallel which combined the first two Virtual Instruments, alongside allowing the sequence of values to control the mass flow controllers.

From Honours report: " " " Figure 12 gives the right side of the front panel of the LabView VI sample with vapour.VI, which letsus preset an autonomously-performed vapour sensing sequence. Each row in each array module corresponds to a differennest step in this sequence. The 'howManySteps' module lets us set how many of these steps are performed. The 'Durations Array' module determines the length of time in seconds each step is performed over. The 'Carrier Flows Array' and 'Dilution Flows Array' modules let us set the carrier flow and dilution flow, respectively, in standard cubic centimetres per minute (sccm) through the gas rig at each step. The carrier flow pushes analyte vapour into the vapour-sensing device chamber, while dilution flow is used to modify the flow behaviour of the analyte vapour entering the chamber. The vapour sensing sequence as depicted in Figure 12 was used for all vapour sensing runs in this investigation. At the end of the sequence, the data collected about the vapour sensing process was saved as an .lvm file. " " "

C.2. Future Improvements

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