

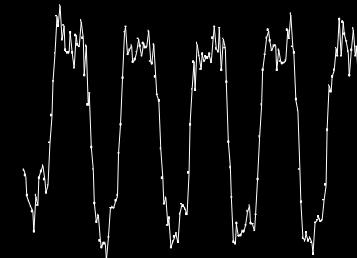
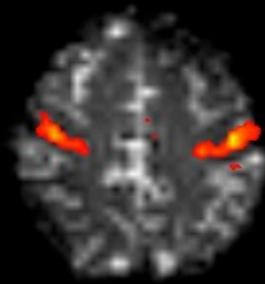
The Spatial, Temporal and Interpretive Limits of Functional MRI

Peter A. Bandettini, Ph.D

Unit on Functional Imaging Methods
Laboratory of Brain and Cognition
National Institute of Mental Health

Categories of Questions Asked with fMRI

Where?



When?

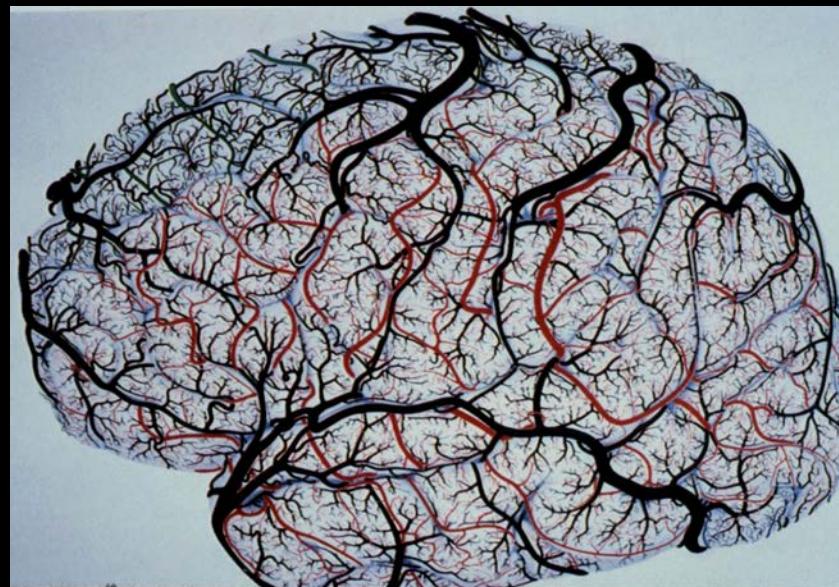
How much?

How to get the brain to do what we want it to
do in the context of an fMRI experiment?

(*limitations: time, motion, acoustic noise....*)

A Primary Challenge:

...to make progressively more precise inferences using fMRI without making too many assumptions about non-neuronal physiologic factors.

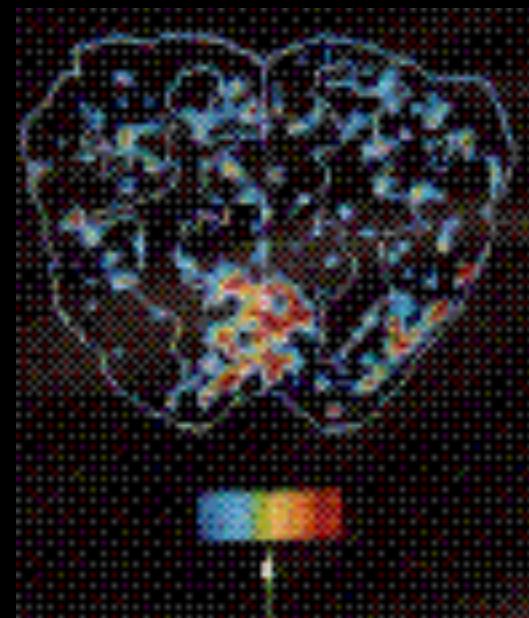
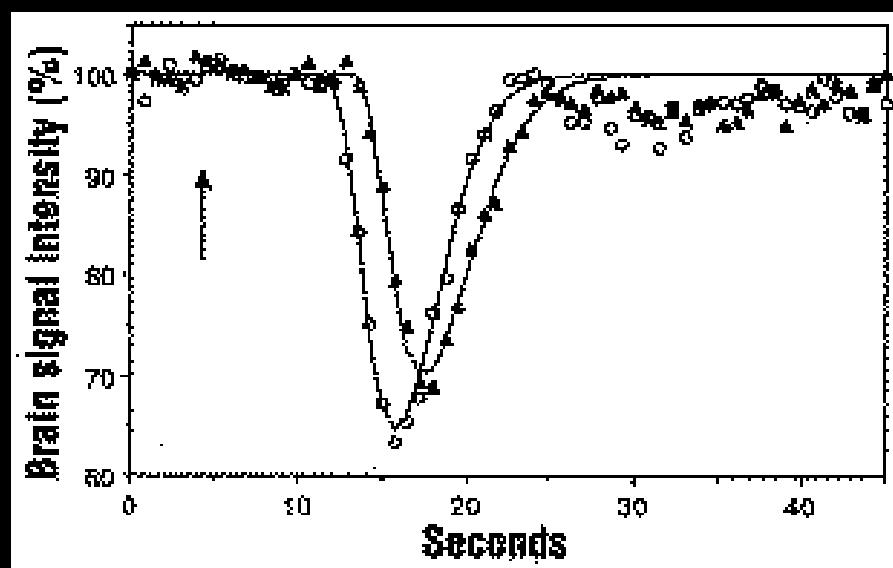
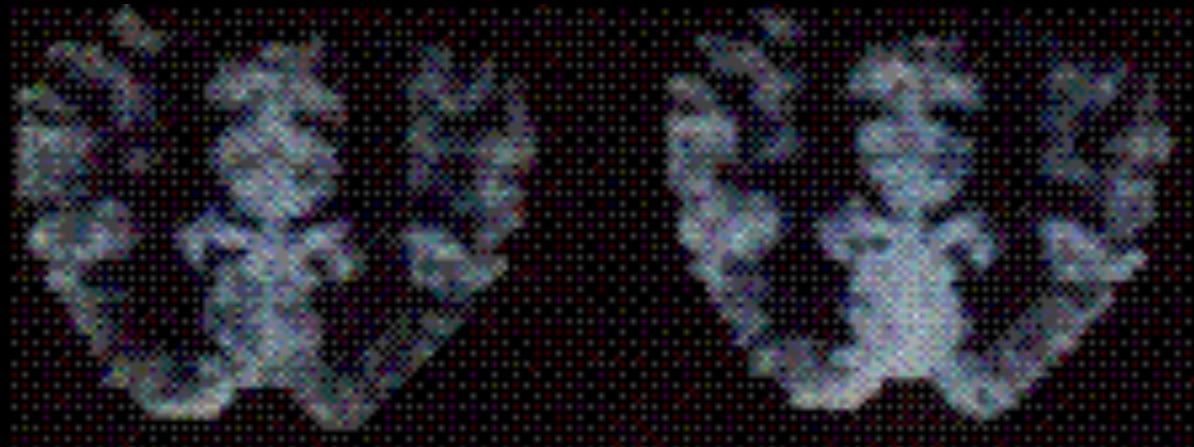


Contrast in Functional MRI

- **Blood Volume**
 - Contrast agent injection and time series collection of T2* or T2 - weighted images
- **BOLD**
 - Time series collection of T2* or T2 - weighted images
- **Perfusion**
 - T1 weighting
 - Arterial spin labeling

Resting

Active

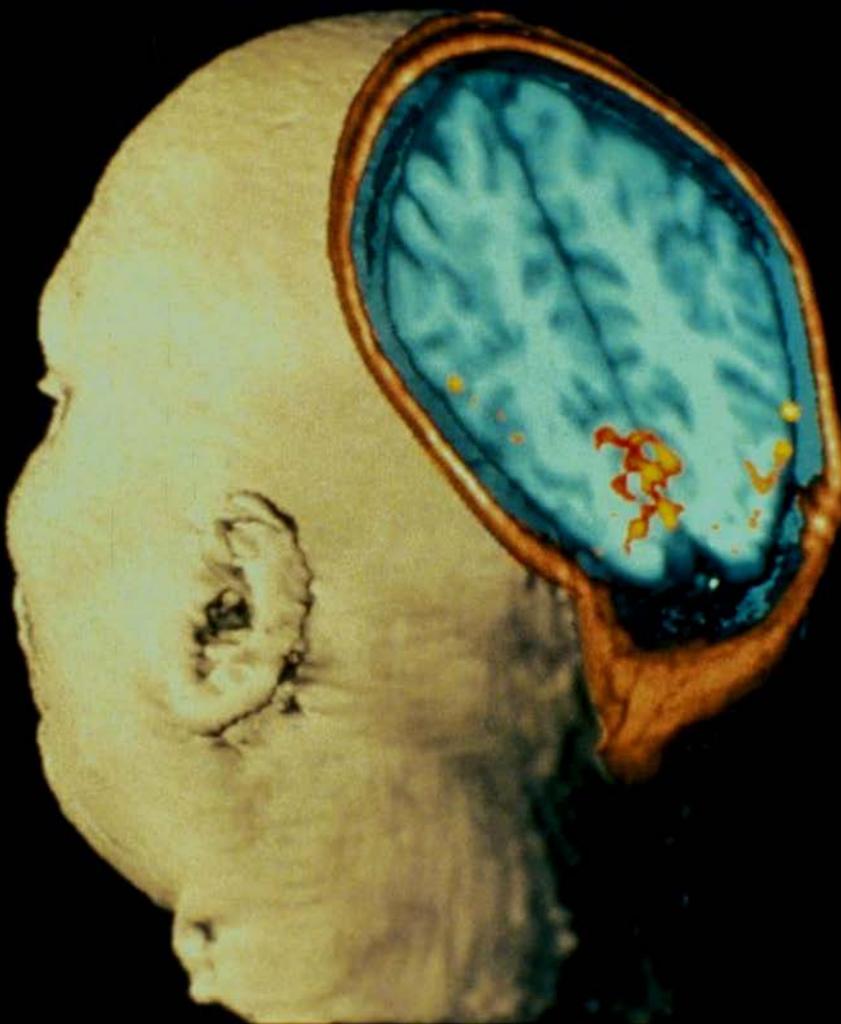


Photic Stimulation

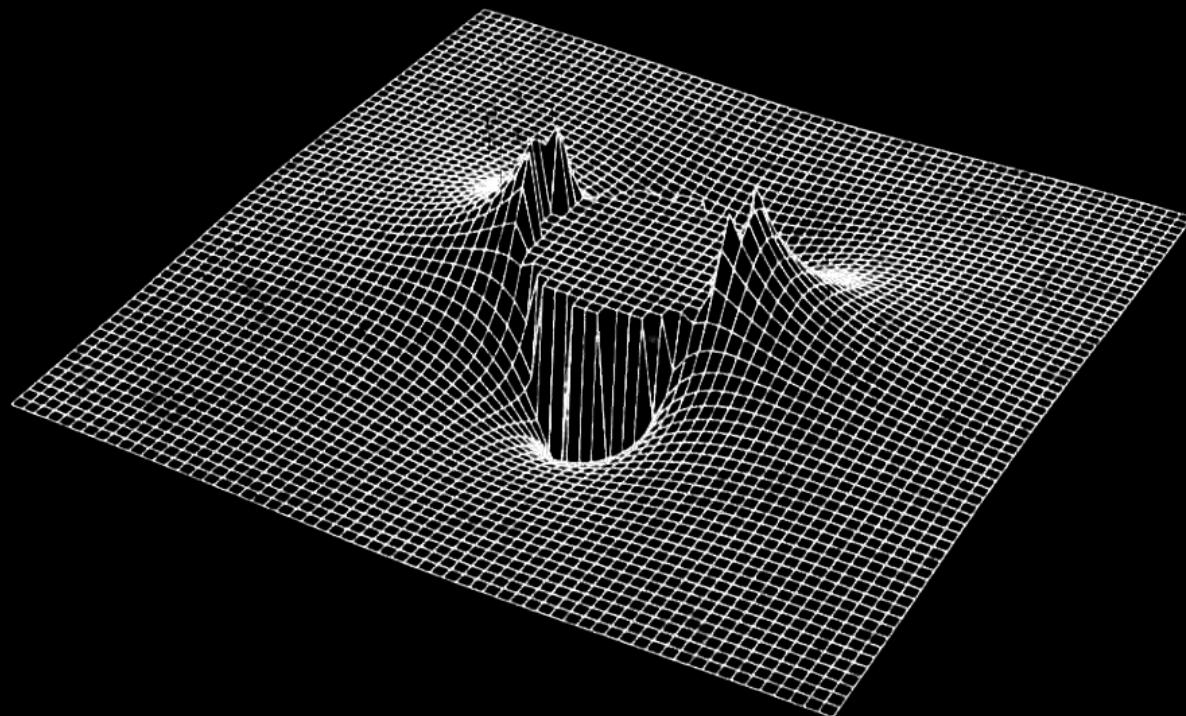
MRI Image showing
activation of the
Visual Cortex

From Belliveau, et al.
Science Nov 1991

MSC - perfusion

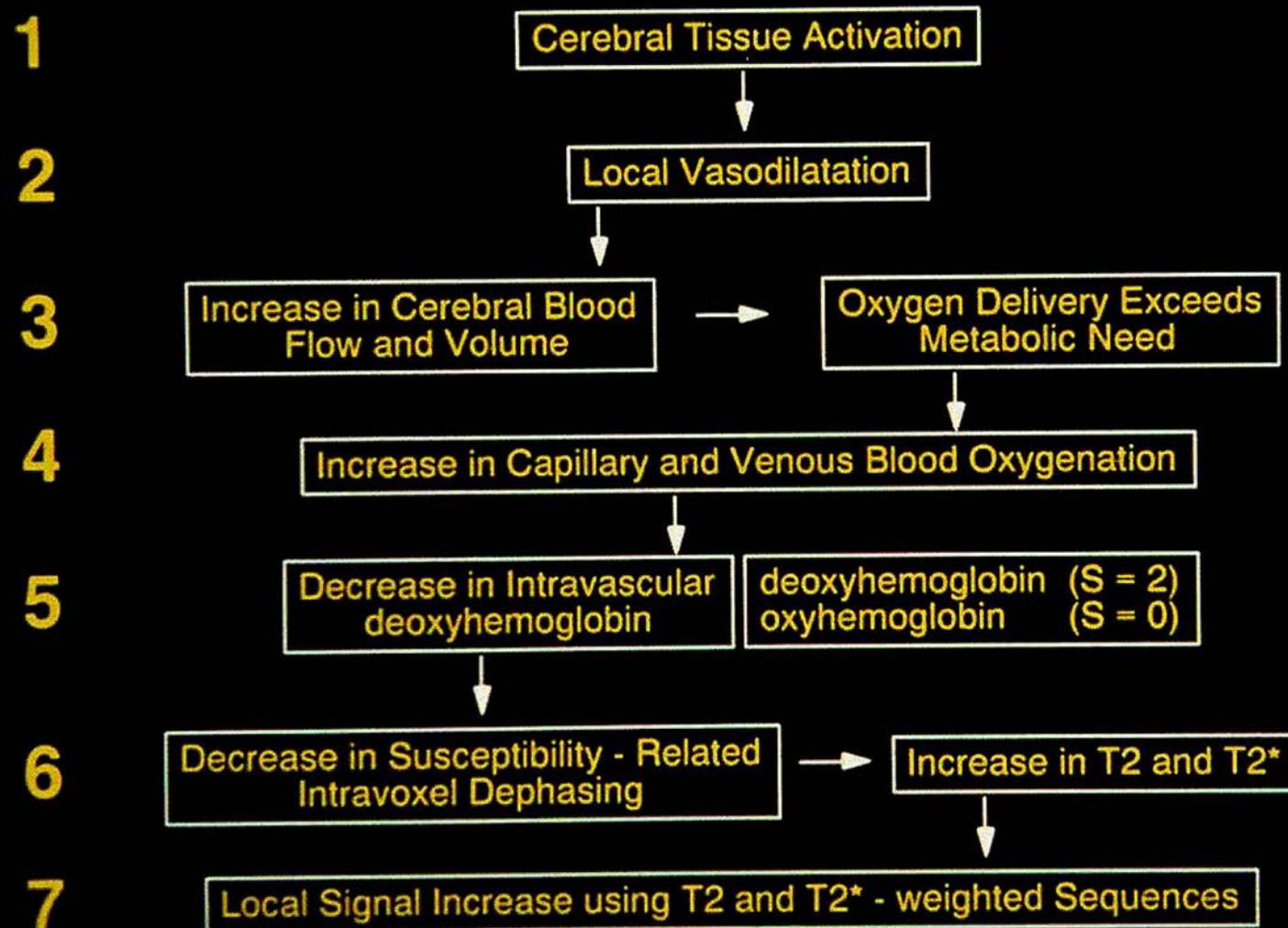


Susceptibility-Induced Field Distortion in the
Vicinity of a Microvessel \perp to B_0 .

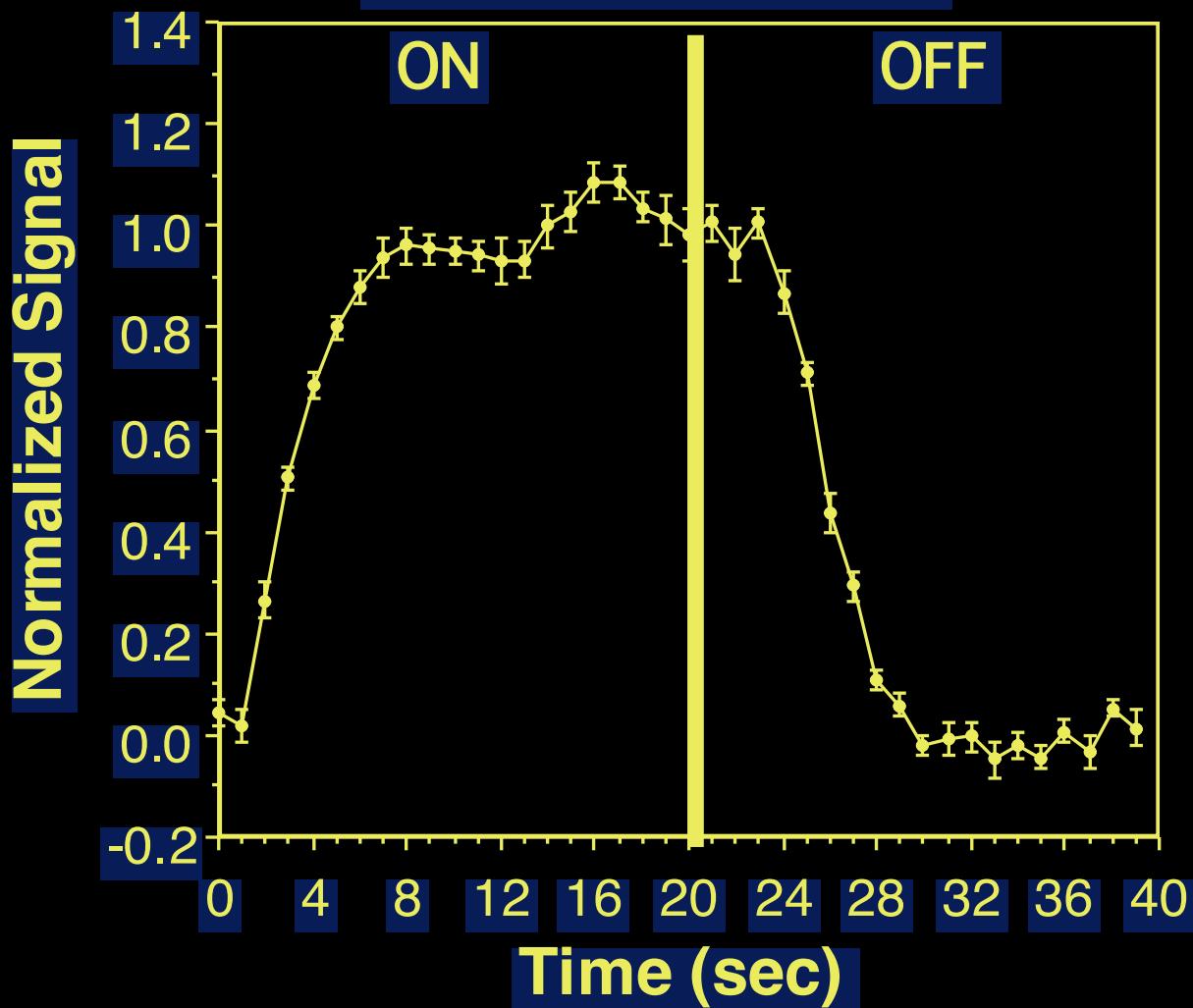


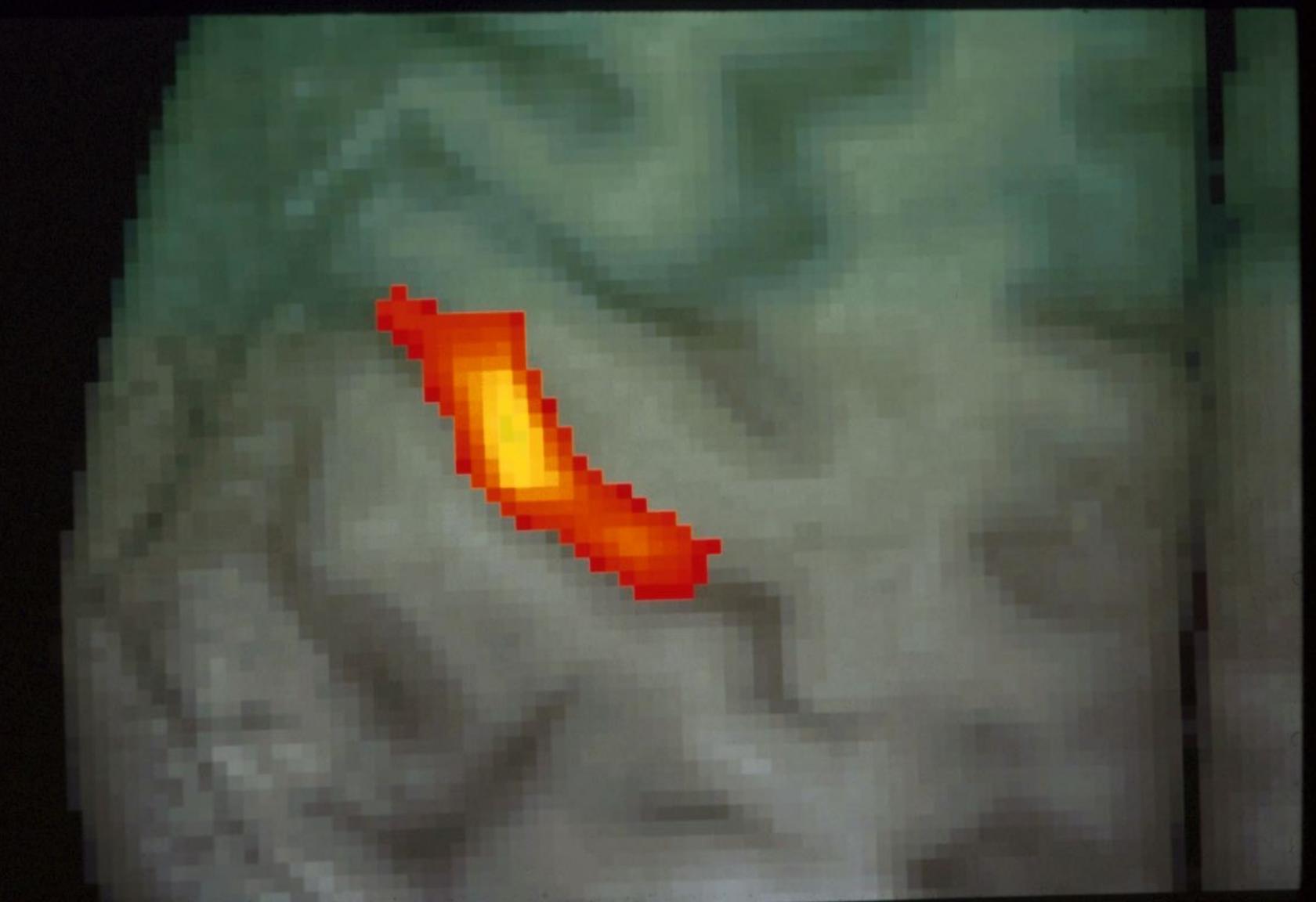


BOLD Contrast in the Detection of Neuronal Activity



Primary Motor Cortex: Gradient-Echo EPI

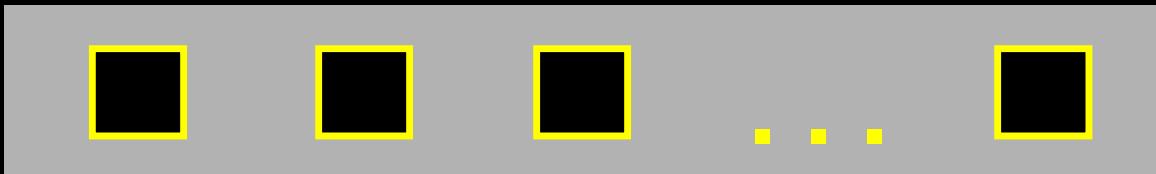
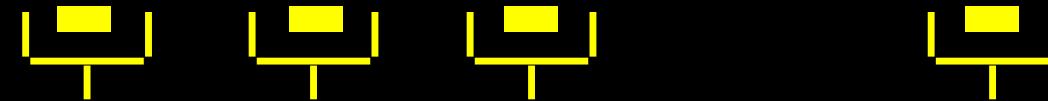
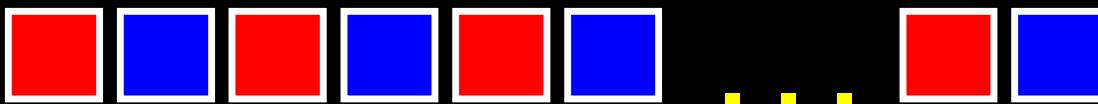
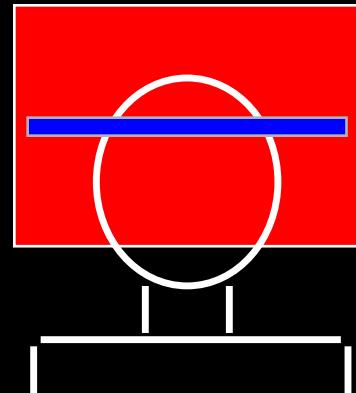
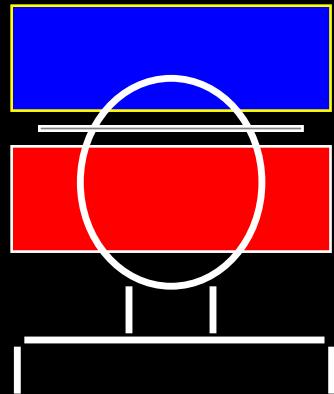




Perfusion / Flow Imaging

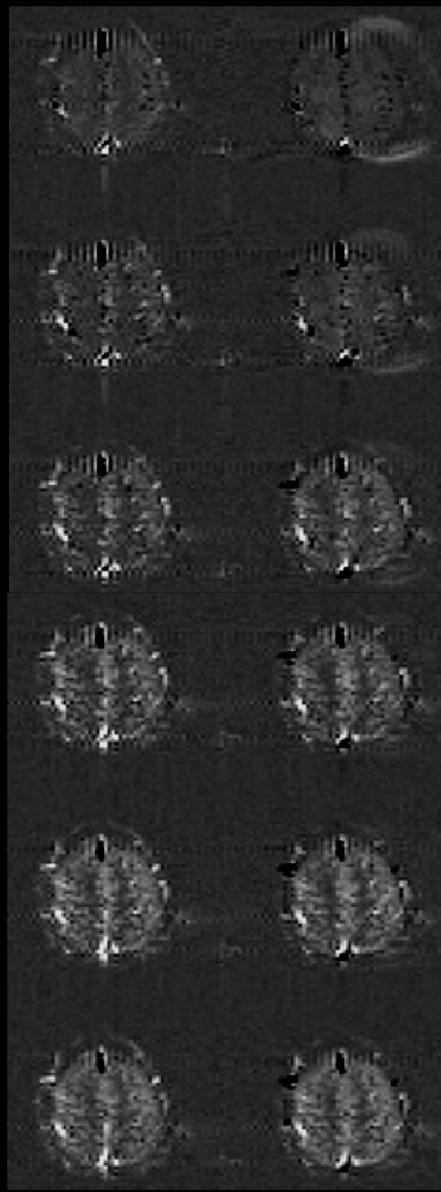
EPISTAR

FAIR



TI (ms) FAIR EPISTAR

200



400

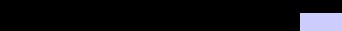
600

800

1000

1200

Volume



- unique information
- baseline information
- multislice trivial

- invasive
- low C / N for func.

BOLD

- highest C / N
- easy to implement
- multislice trivial
- non invasive
- highest temp. res.

- complicated signal
- no baseline info.

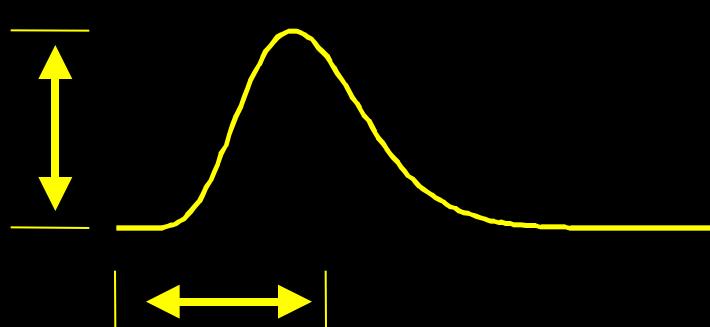
Perfusion

- unique information
- control over ves. size
- baseline information
- non invasive

- multislice non trivial
- lower temp. res.
- low C / N

**Neuronal
Activation**

**Measured
fMRI
Signal**

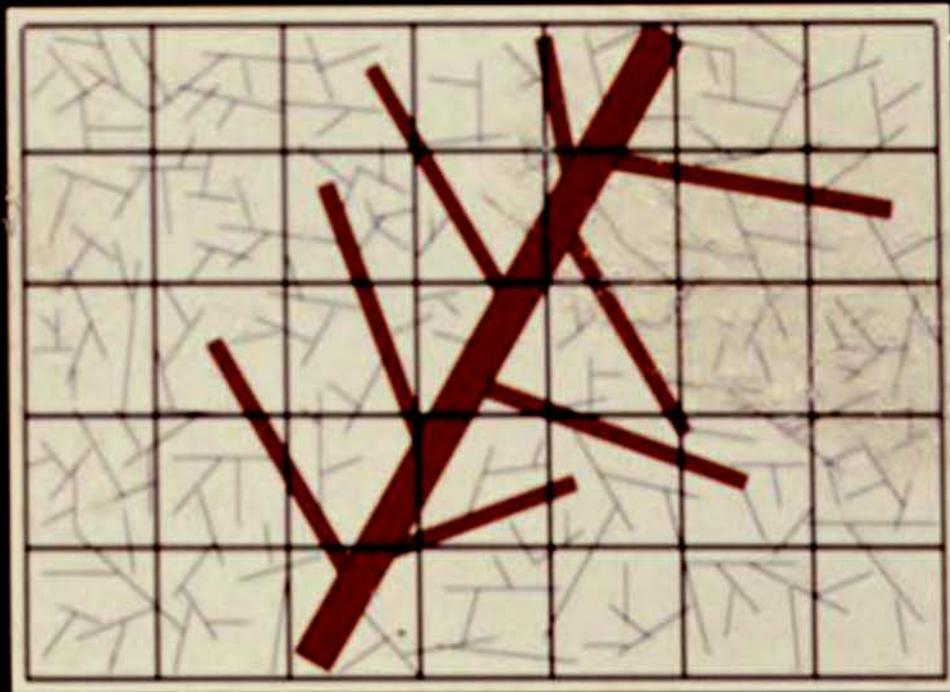
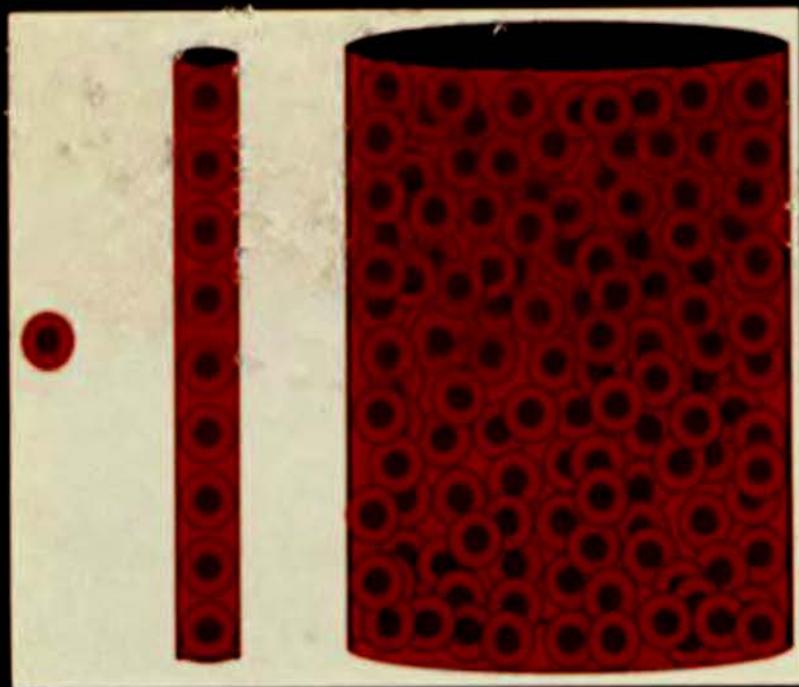


Physiologic Factors

Physiologic Factors that Influence BOLD Contrast

- Blood oxygenation
- Blood volume
- Blood pressure
- Hematocrit
- Vessel size

Coupling:
Flow & CMRO₂



Where and When?

**The resolution is determined by
the cerebral hemodynamics.**

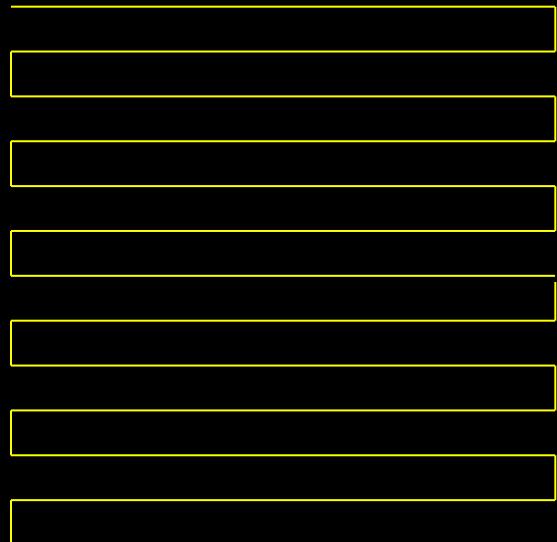
- Know the vasculature at which you are looking.
(or)
- Normalize to the spatial variation in the vasculature.
(or)
- Make several assumptions.

Single Shot Imaging

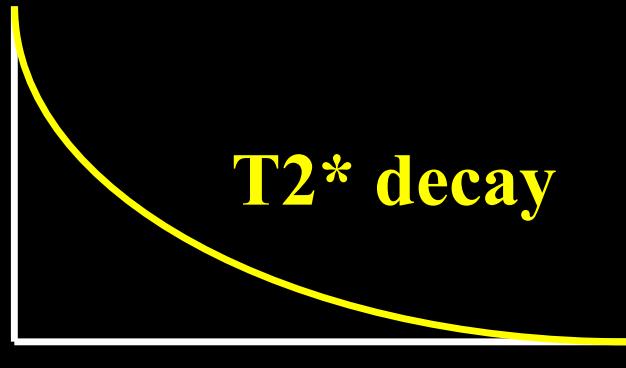


EPI Readout Window

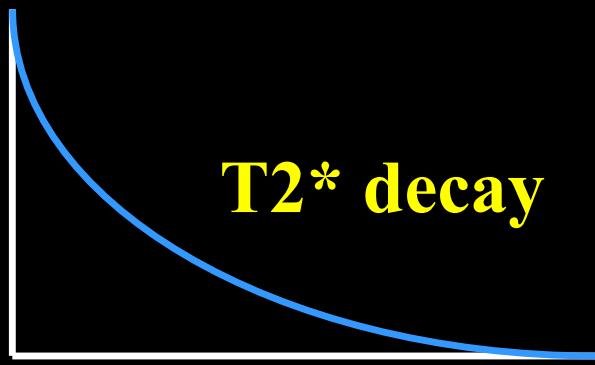
≈ 20 to 40 ms



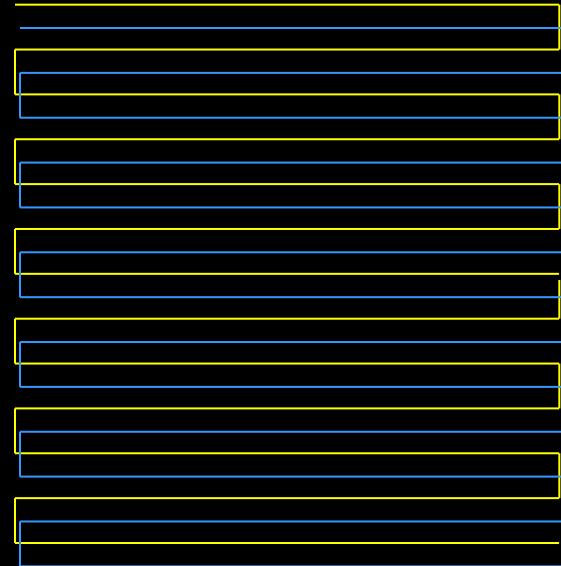
Multishot Imaging



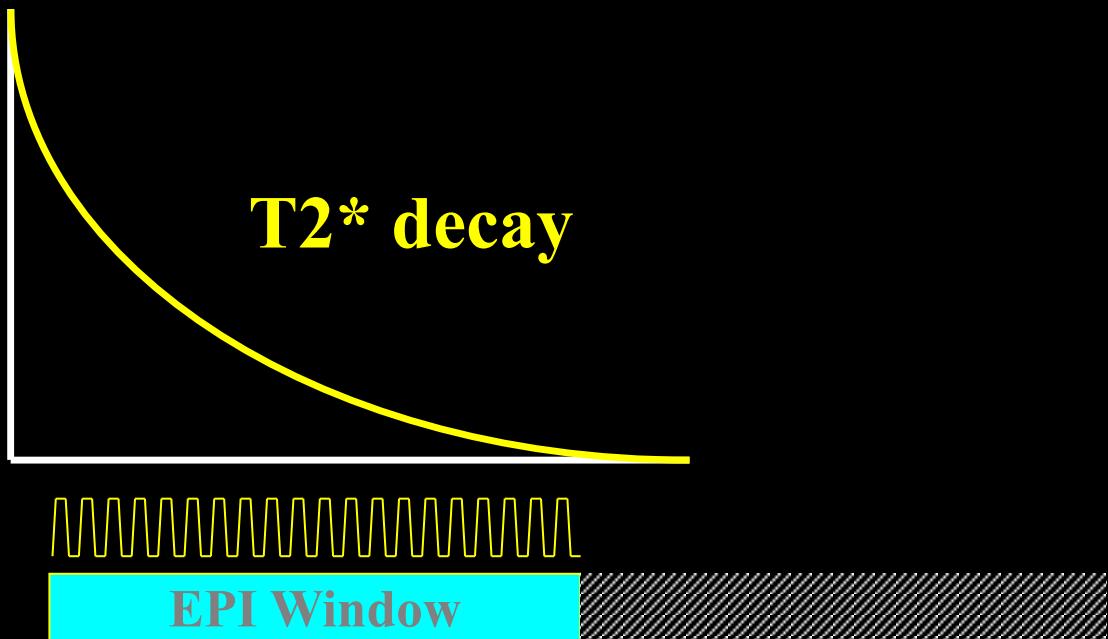
$T2^*$ decay



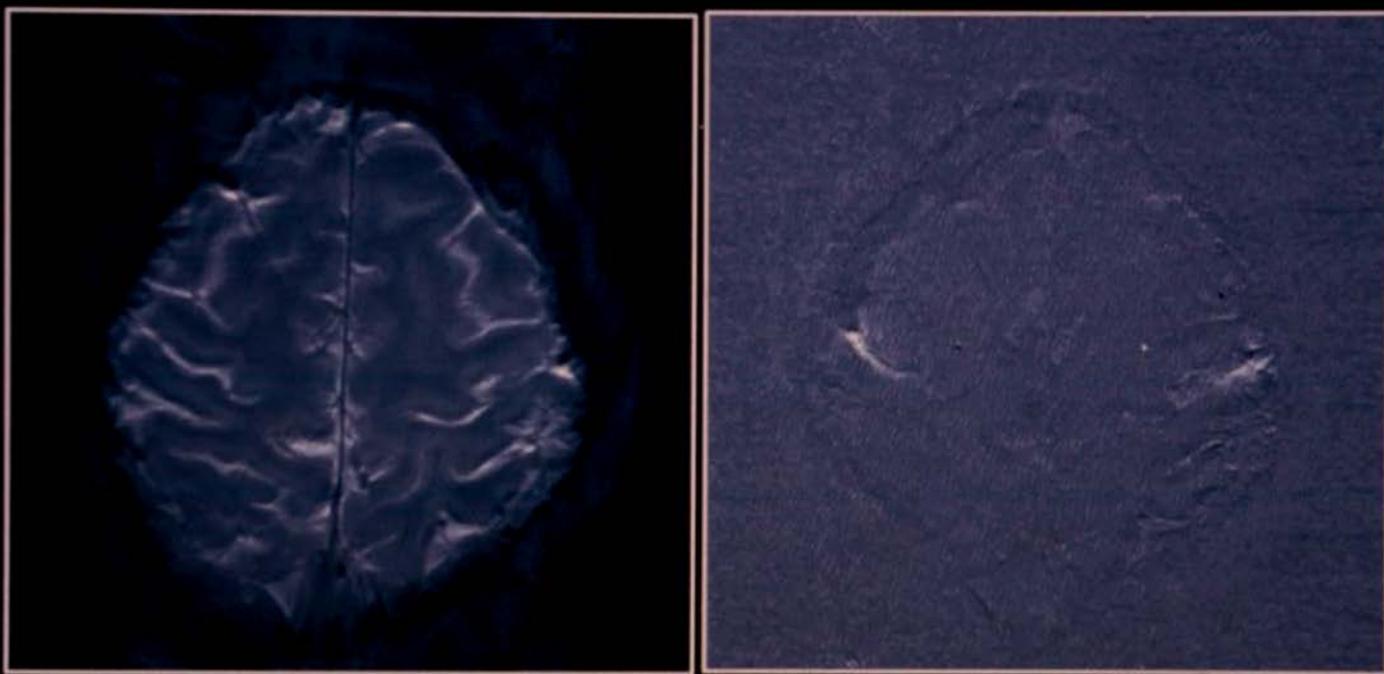
$T2^*$ decay



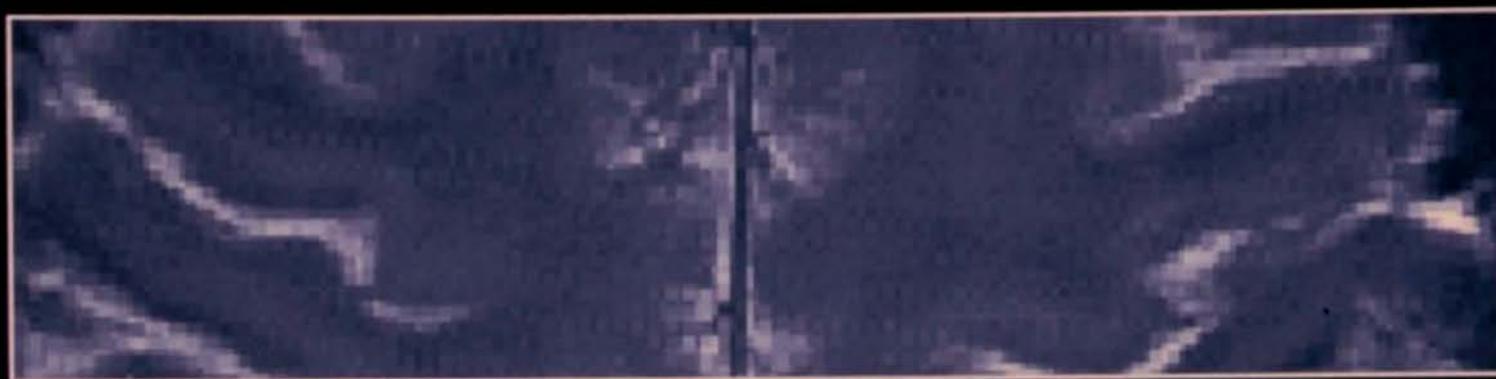
Partial k-space imaging

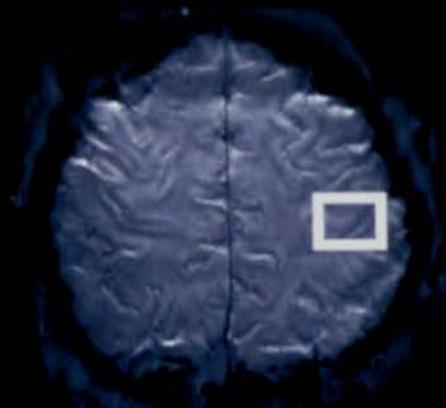


**Single - Shot EPI at 3T:
Half NEX, 256 x 256, 16 cm FOV**



**Single - Shot EPI at 3T:
Half NEX 256 x 256, 16 cm FOV**





64 x 64

96 x 96

128 x 128

192 x 192

256 x 256

%



C/N



2.5 mm²

1.67 mm²

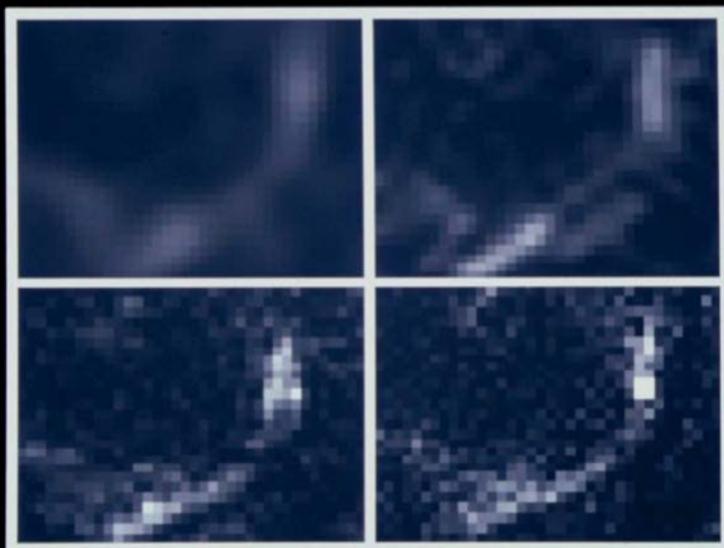
1.25 mm²

0.83 mm²

0.62 mm²

Fractional Signal Change

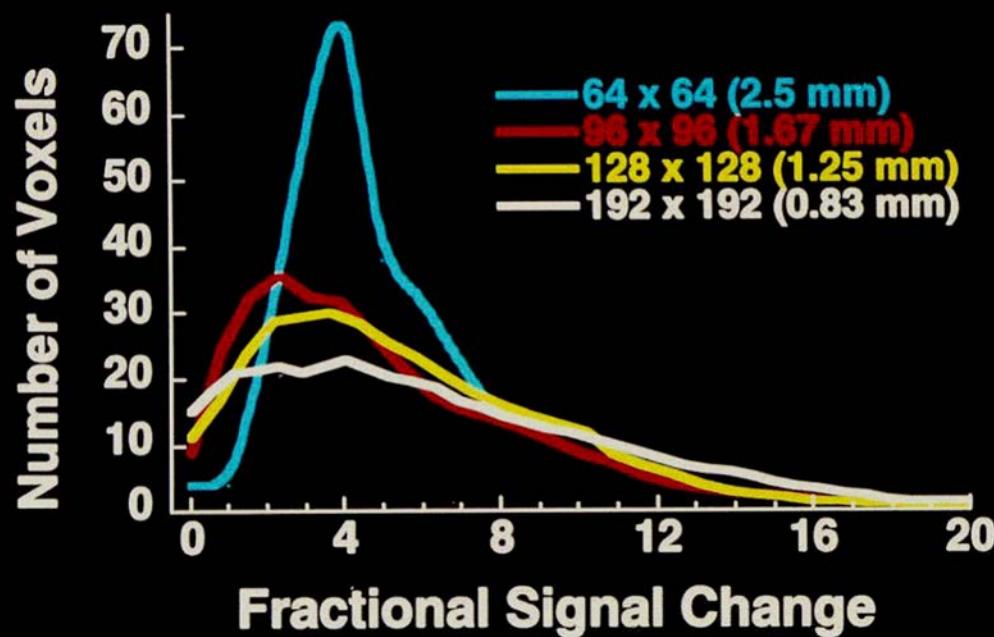
2.5 mm^2



1.25 mm^2

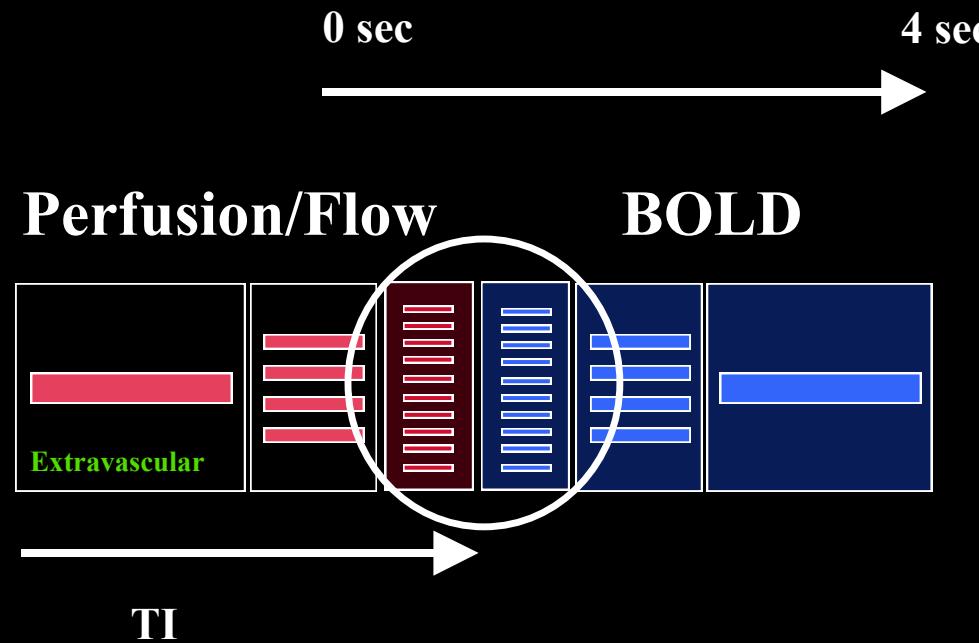
0.83 mm^2

0.62 mm^2



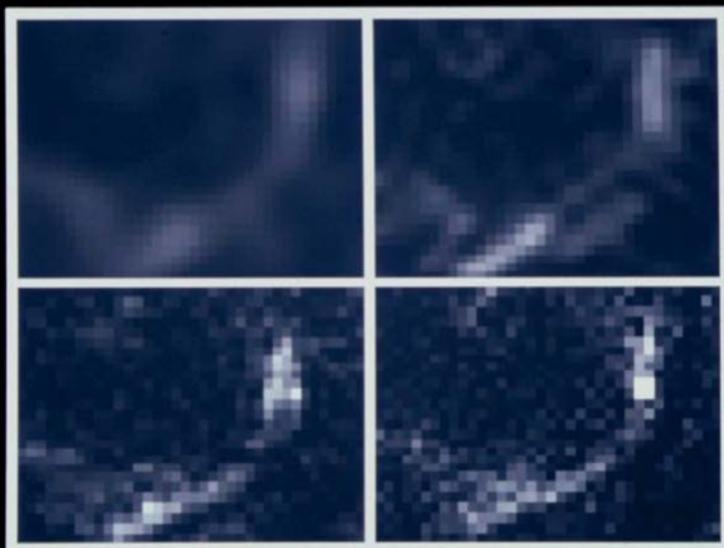
Pulse sequence based methods for increasing spatial and temporal resolution

- Spin-echo
- ASL
- Diffusion weighting
- Threshold based on magnitude



Fractional Signal Change

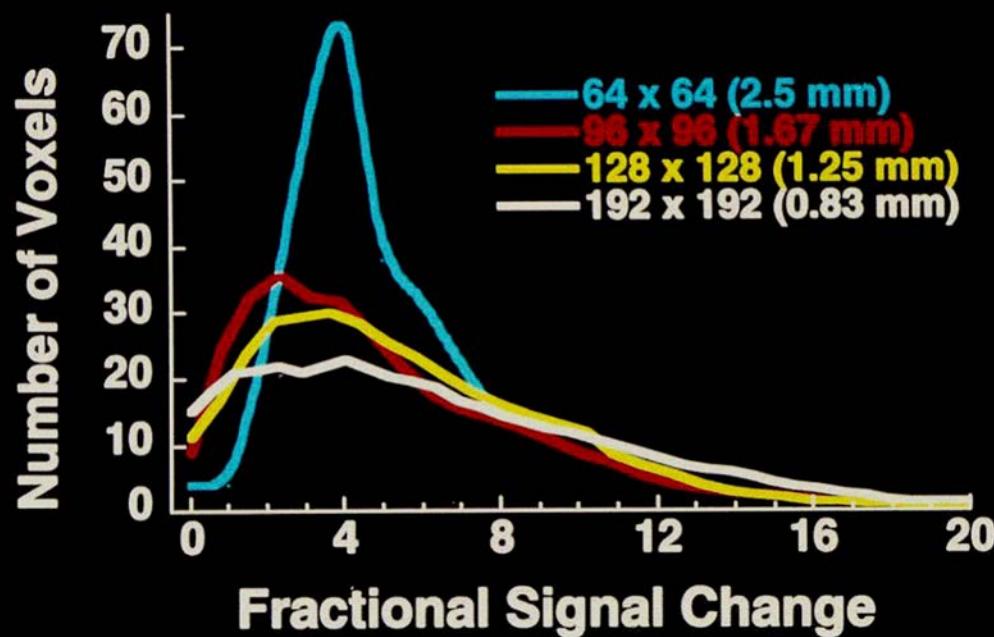
2.5 mm^2



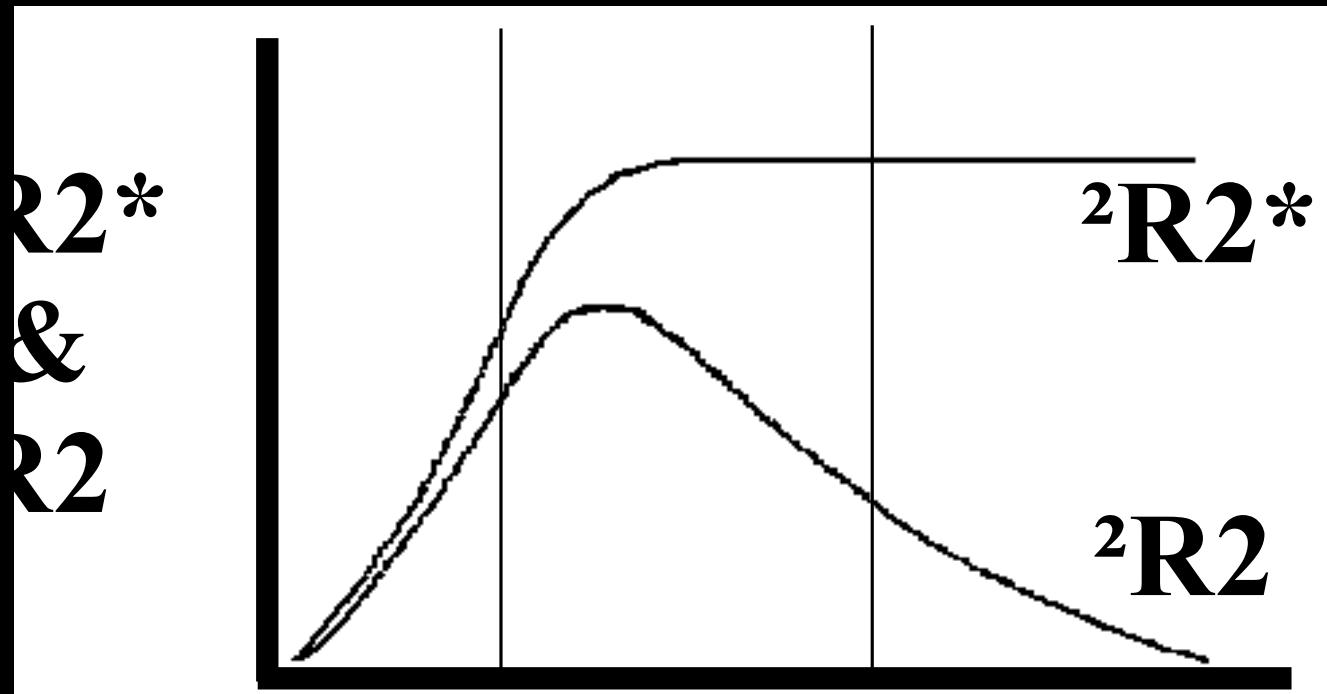
1.25 mm^2

0.83 mm^2

0.62 mm^2



Spin echo vs. Gradient echo



compartment
radius:

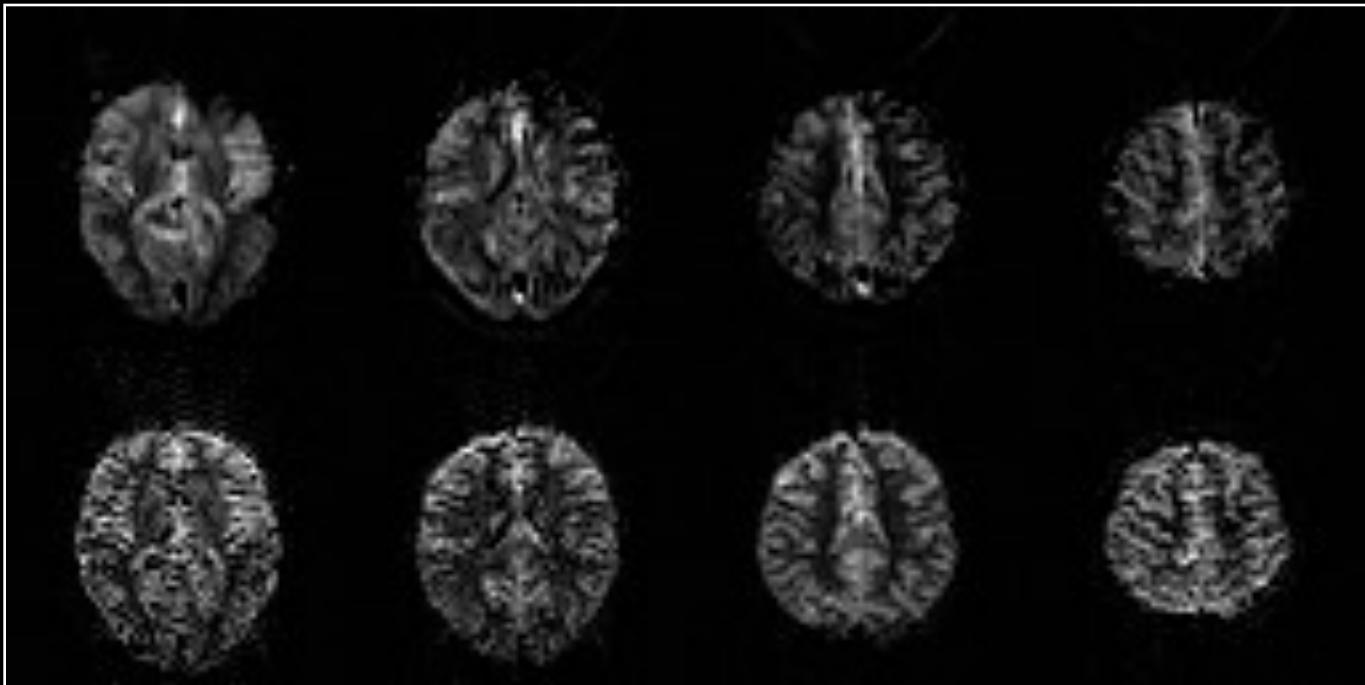
$< 3 \mu\text{m}$

$3 \text{ to } 15 \mu\text{m}$

$> 15 \mu\text{m}$

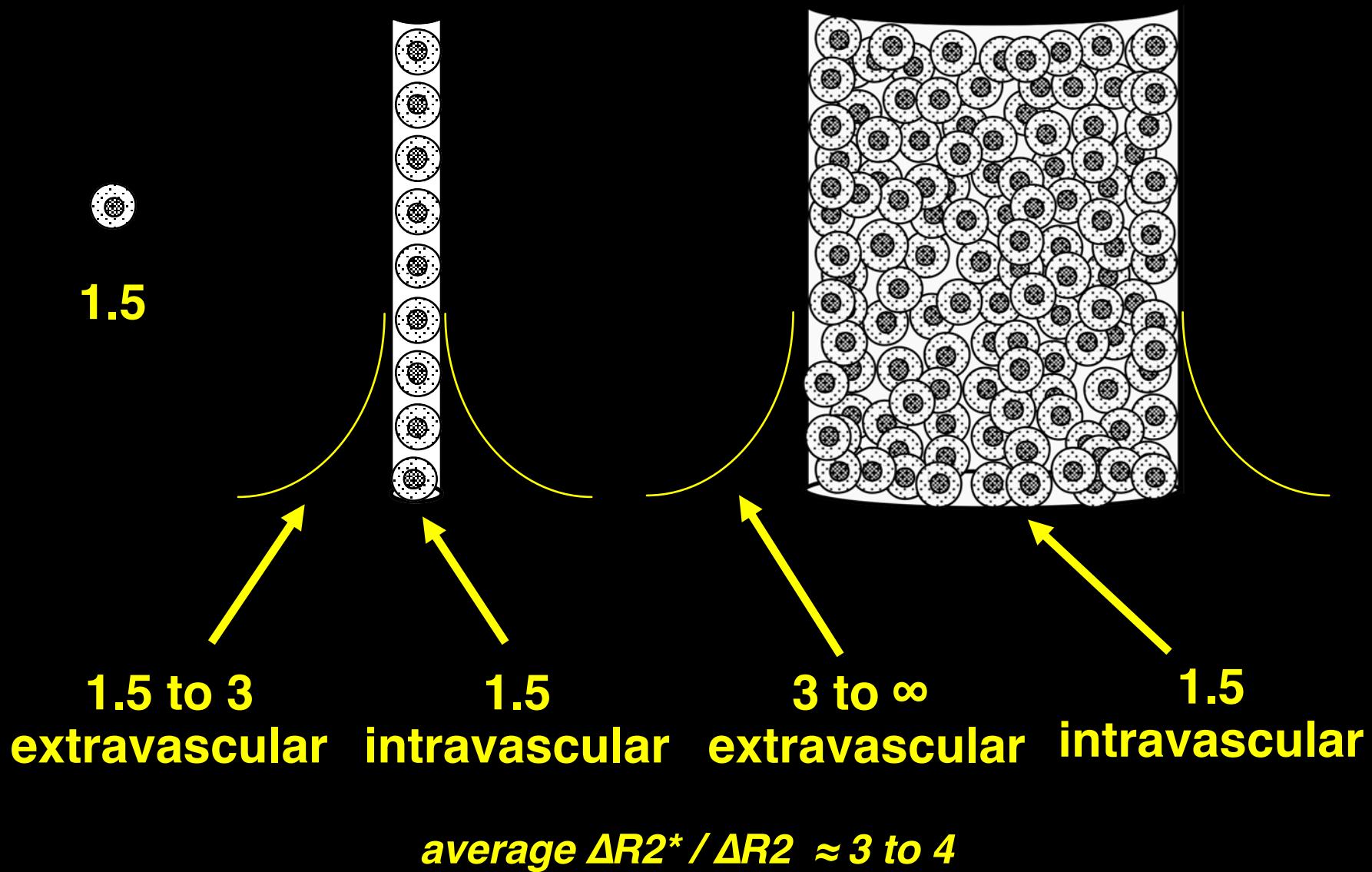
GE
TE = 30 ms

SE
TE = 110 ms



Spin-echo??

$\Delta R2^* / \Delta R2$



3T

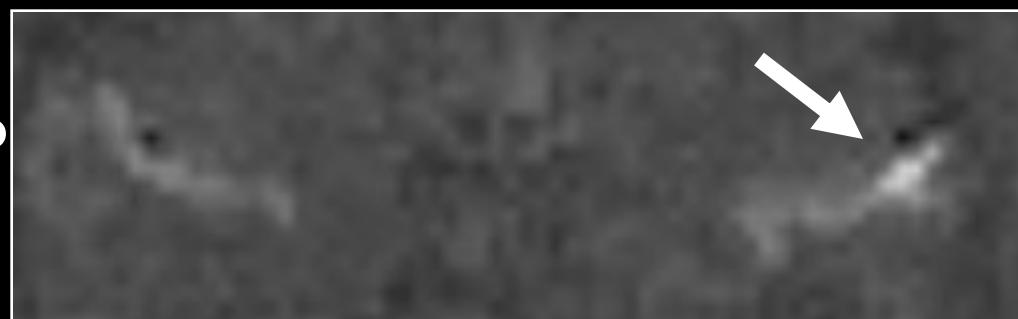
Spin-Echo
TE = 105 ms
TR = ∞



Gradient-Echo
TE = 50 ms



Gradient-Echo
functional
TE = 50 ms

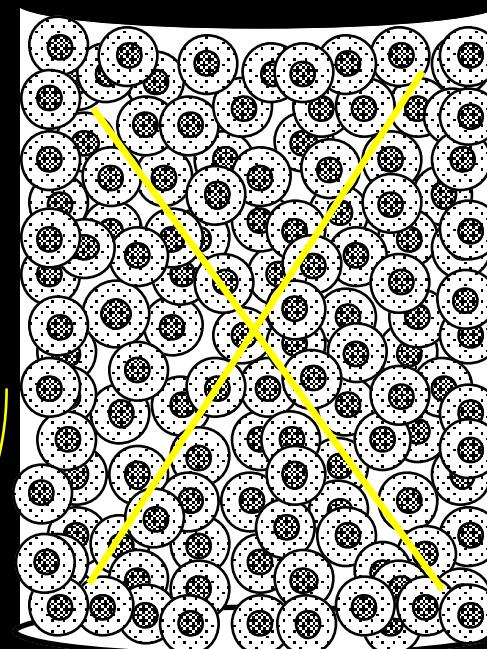
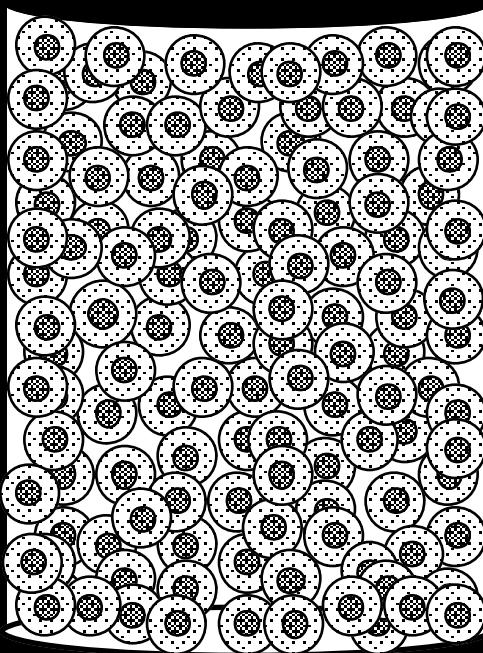


Spin-Echo
functional
TE = 105 ms

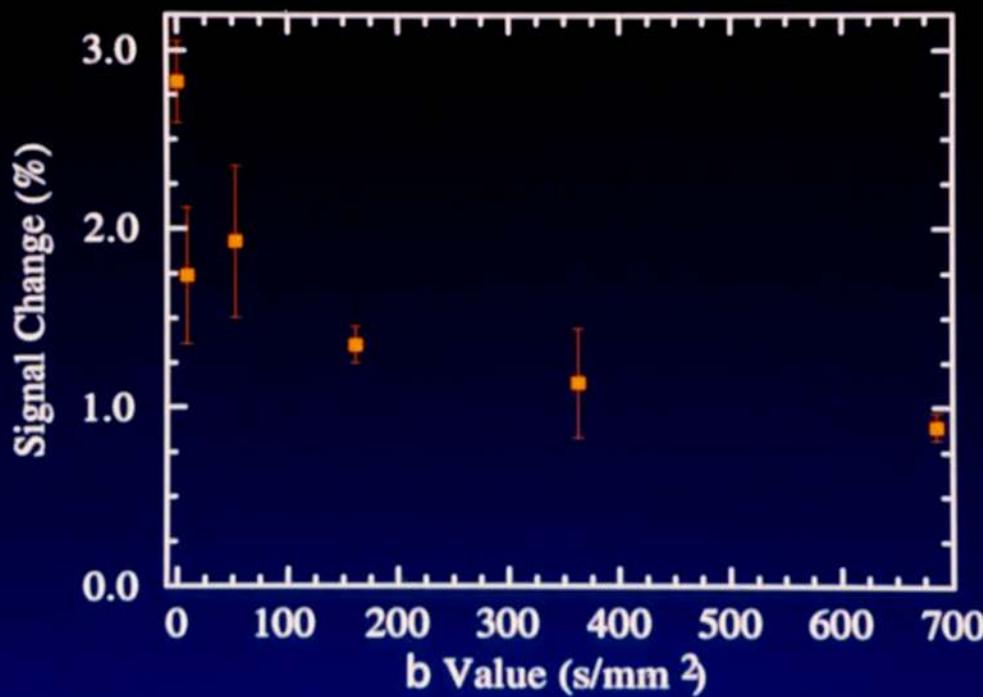


no diffusion weighting

diffusion weighting

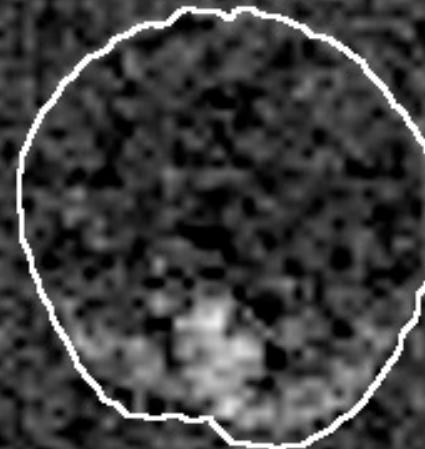
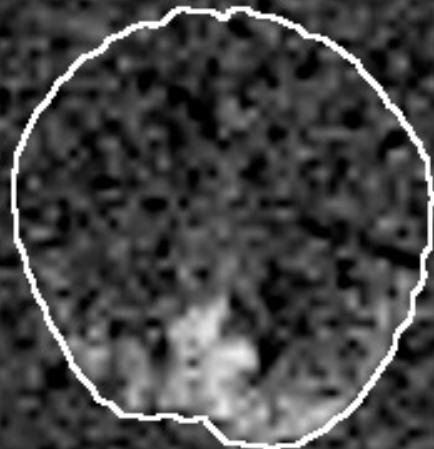


Summary of Diffusion-Weighted fMRI Data



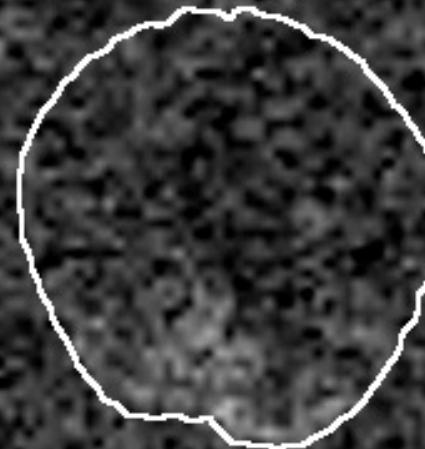
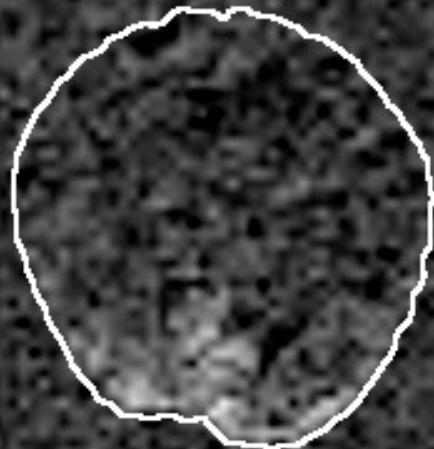
$b = 0$

$b = 10$



$b = 50$

$b = 160$

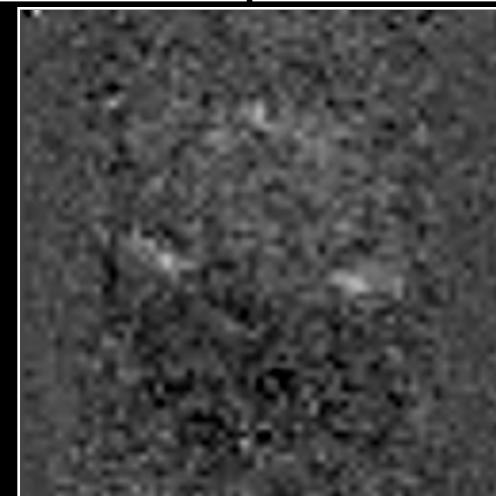
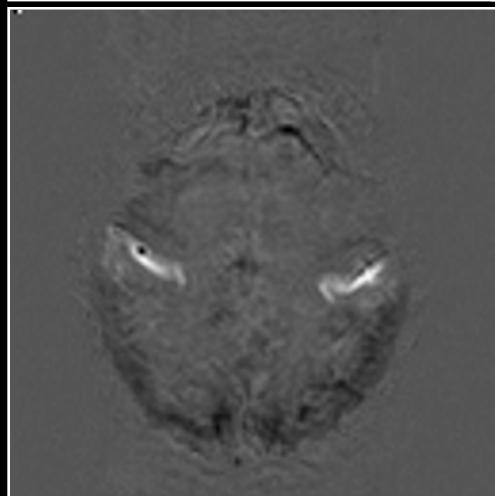
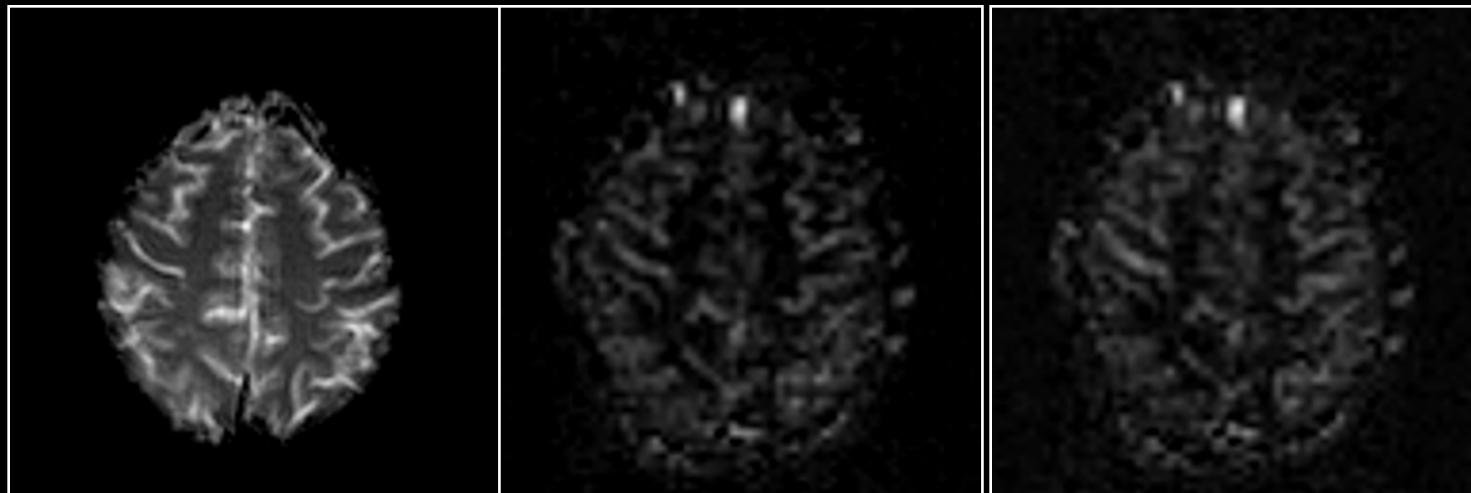


Perfusion

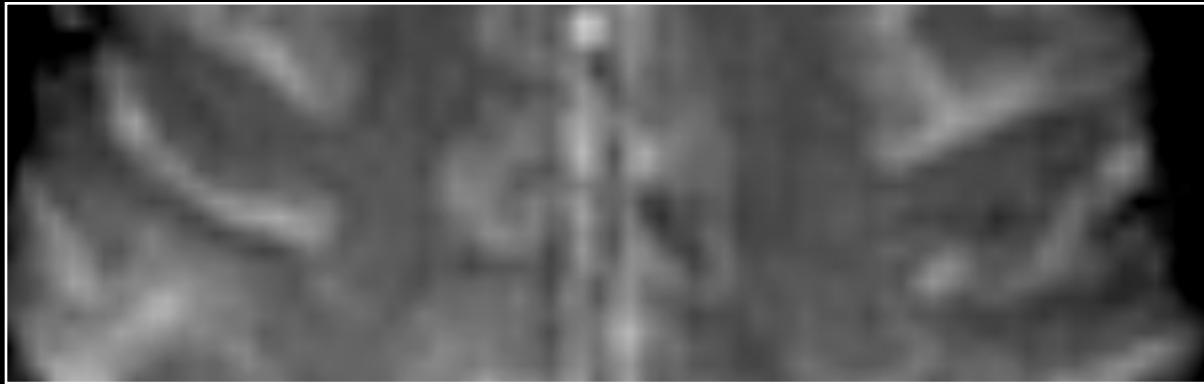
BOLD

Rest

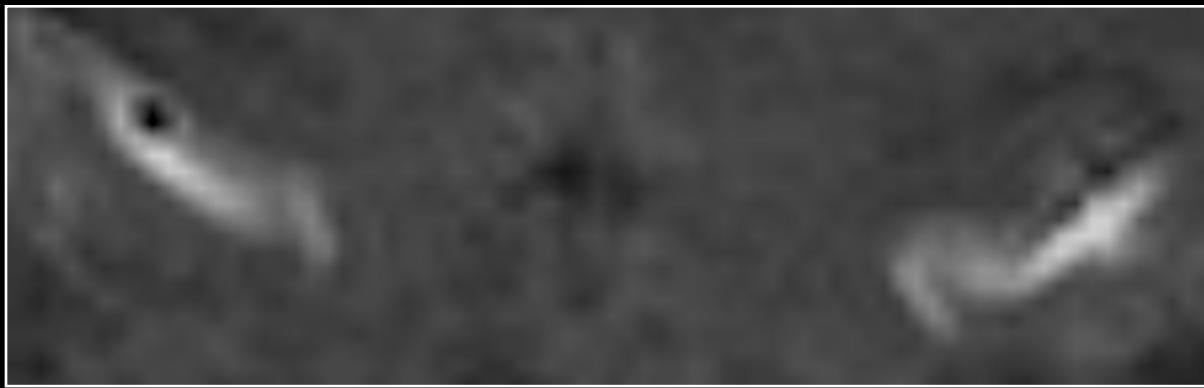
Activation



Anatomy



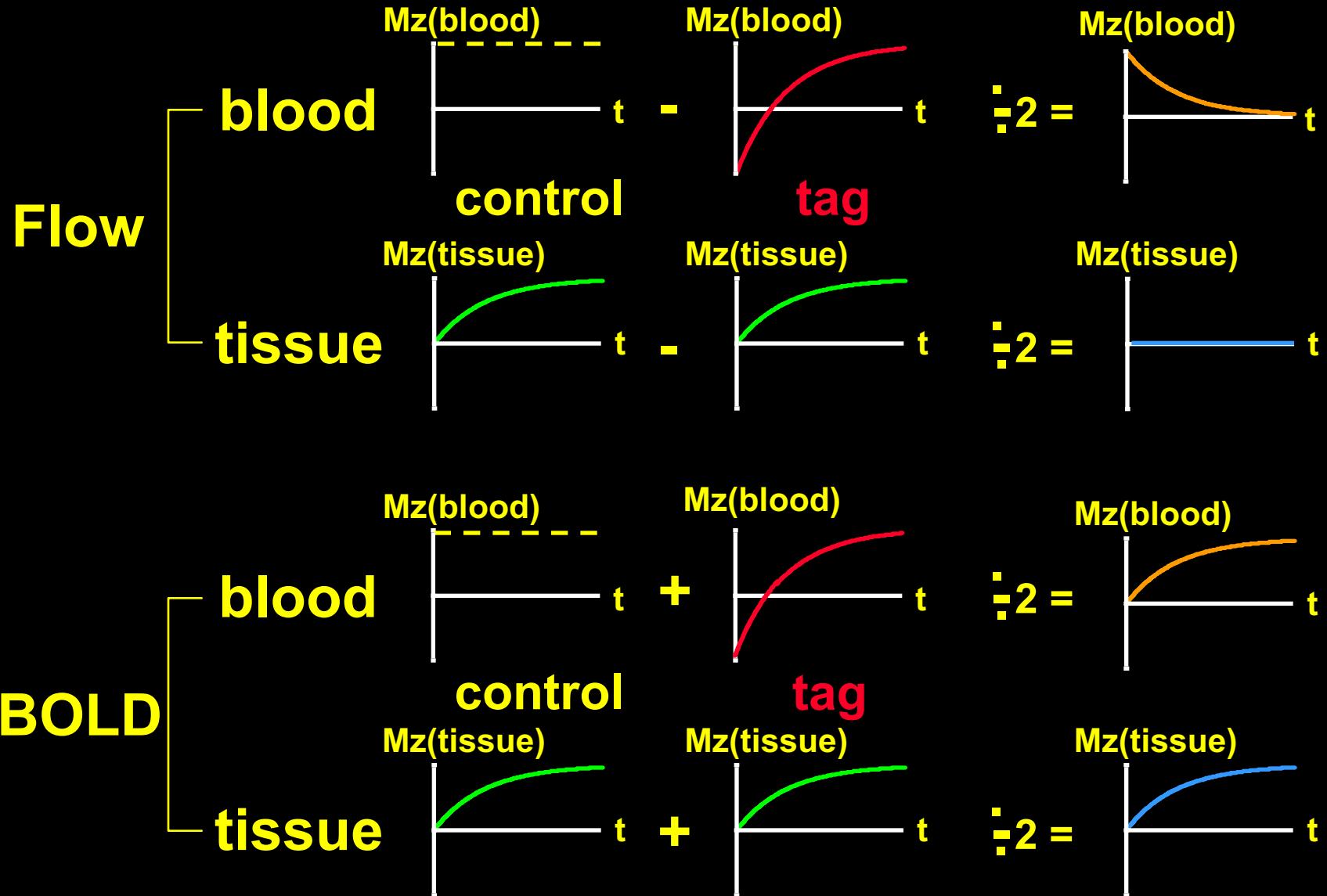
BOLD



Perfusion



Simultaneous Flow and BOLD



Simultaneous BOLD and Perfusion



BOLD



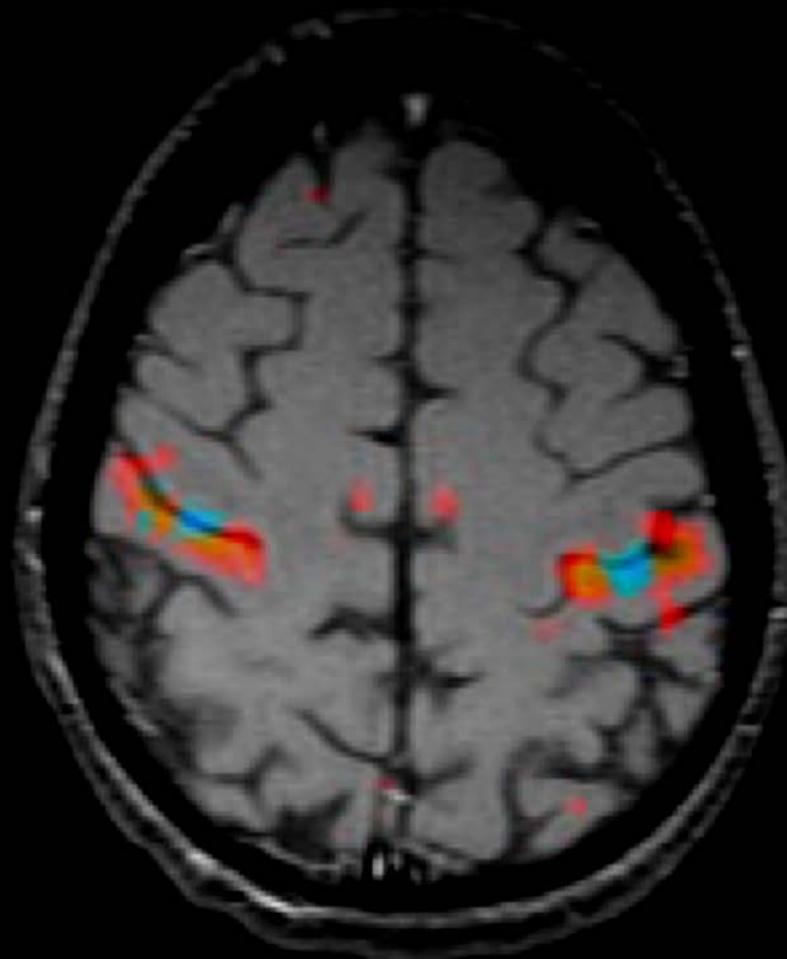
Perfusion



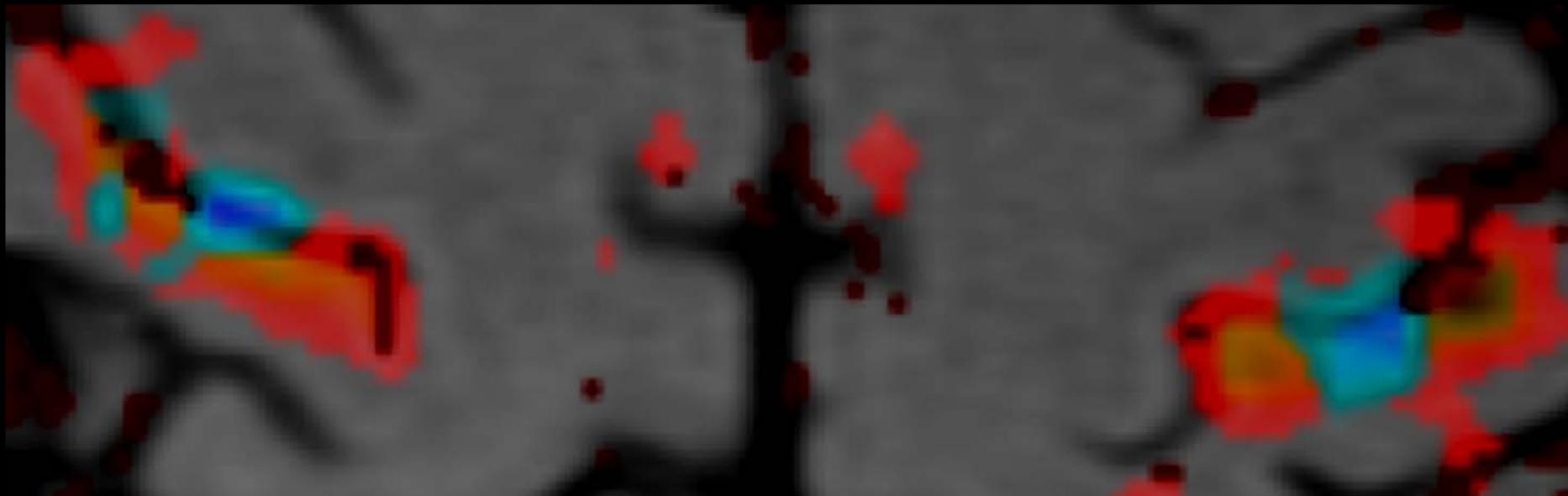
Simultaneous BOLD and Perfusion

perfusion

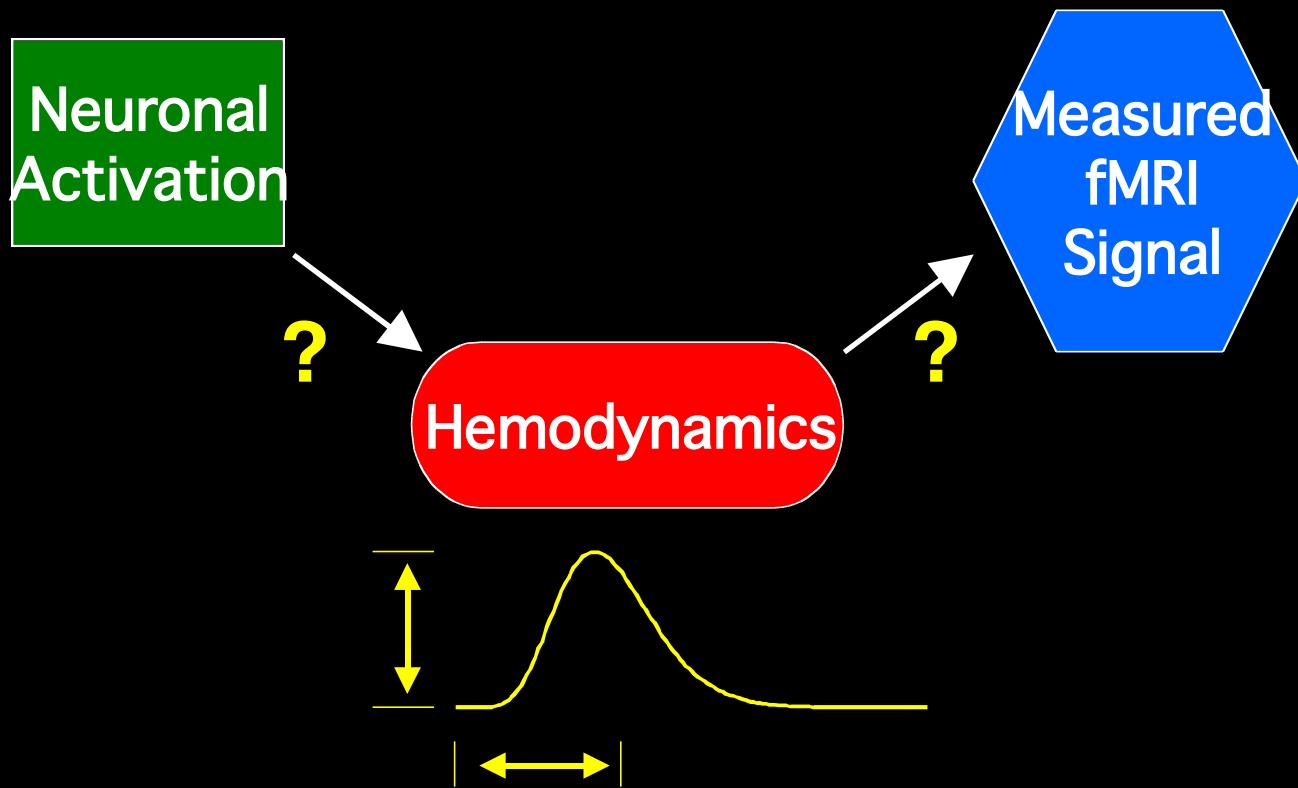
BOLD



Angiogram Perfusion **BOLD**



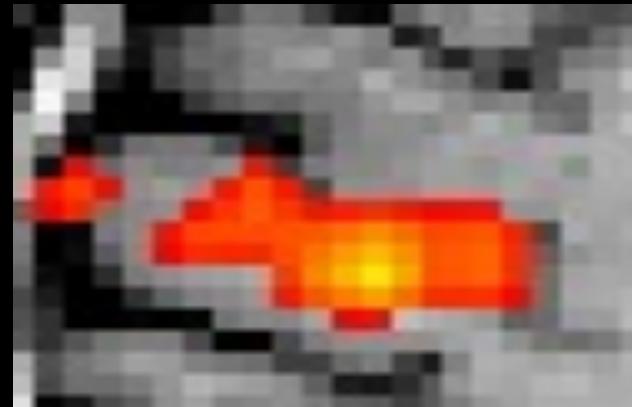
Spatial Normalization



Physiologic Factors

Hypercapnia

T1 - weighted



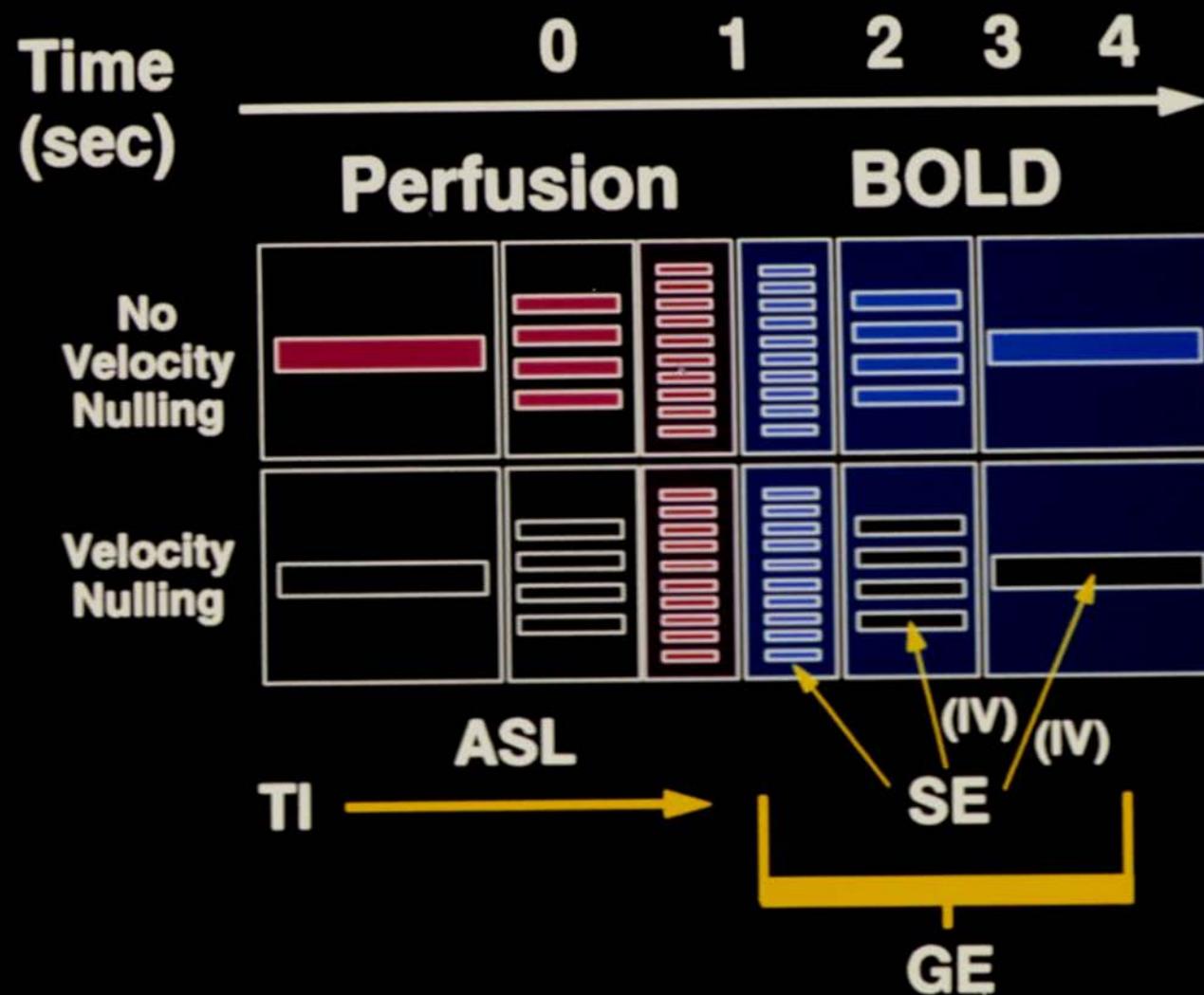
T2* weighted



T1 and T2*
weighted

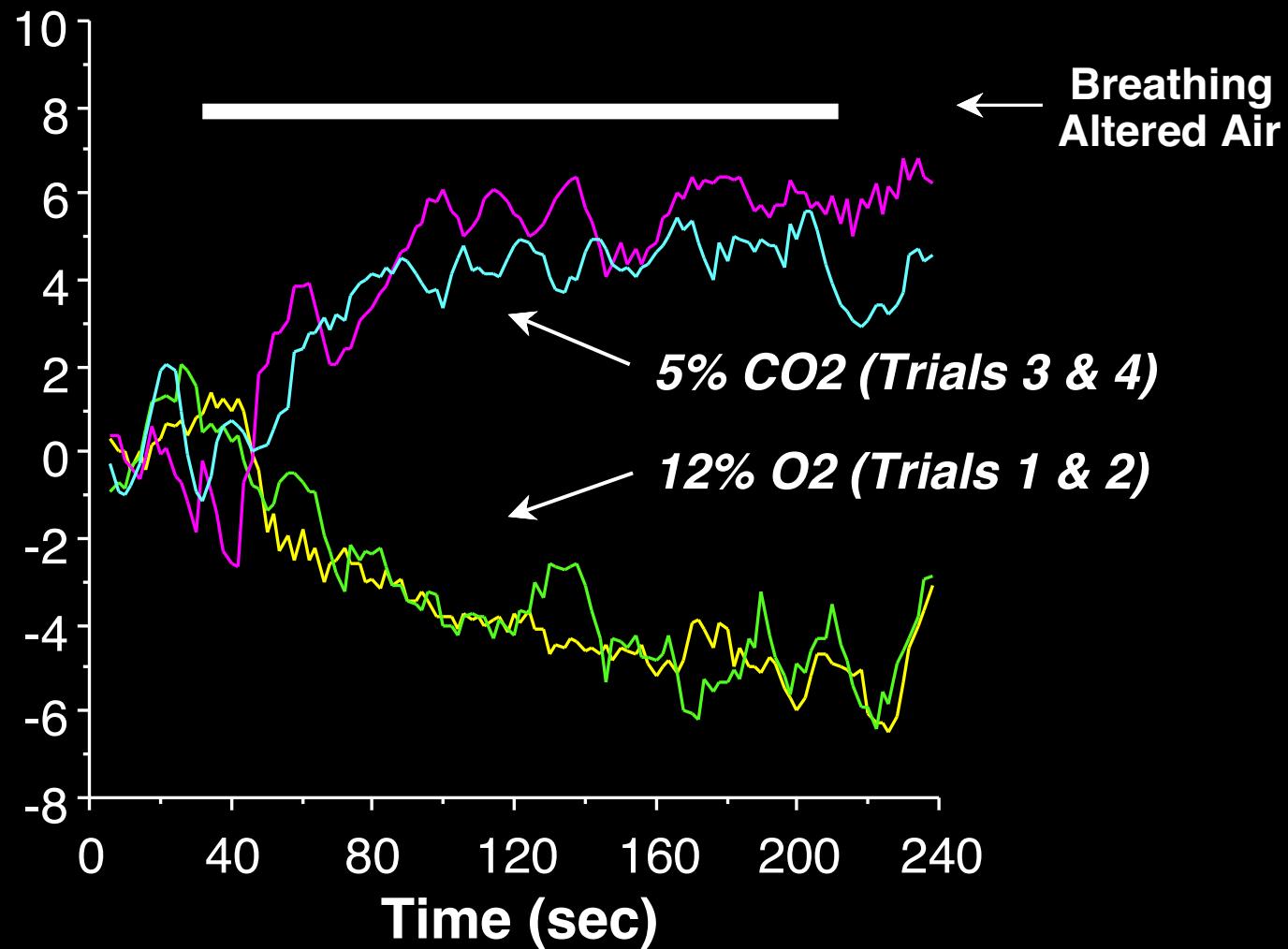


Vascular Sensitization



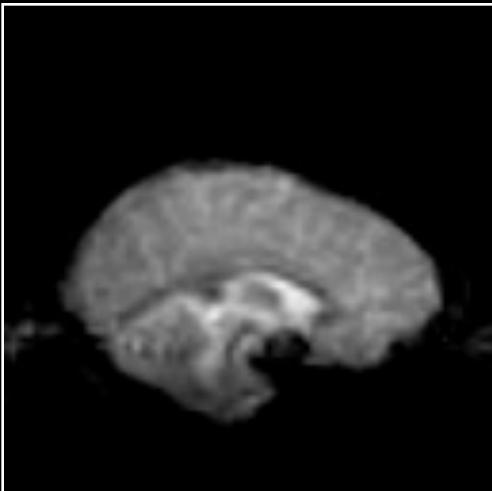
Problems with pulse sequence - based methods for increasing resolution

- Spin-echo (**sensitivity, specificity**)
- Arterial spin-labeling (**sensitivity, time, range**)
- Diffusion weighting (**sensitivity, specificity**)
- Threshold based on magnitude (**sensitivity, specificity**)

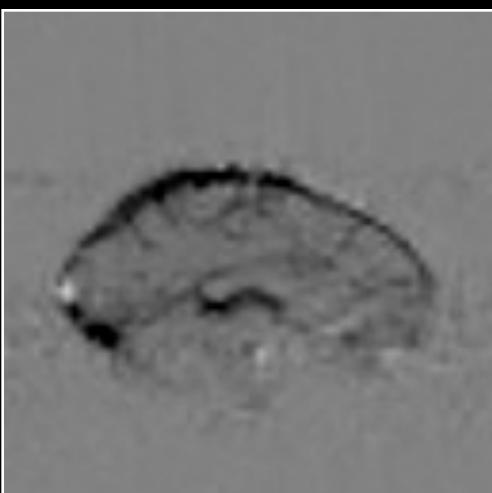


,

Anatomical



12% O₂

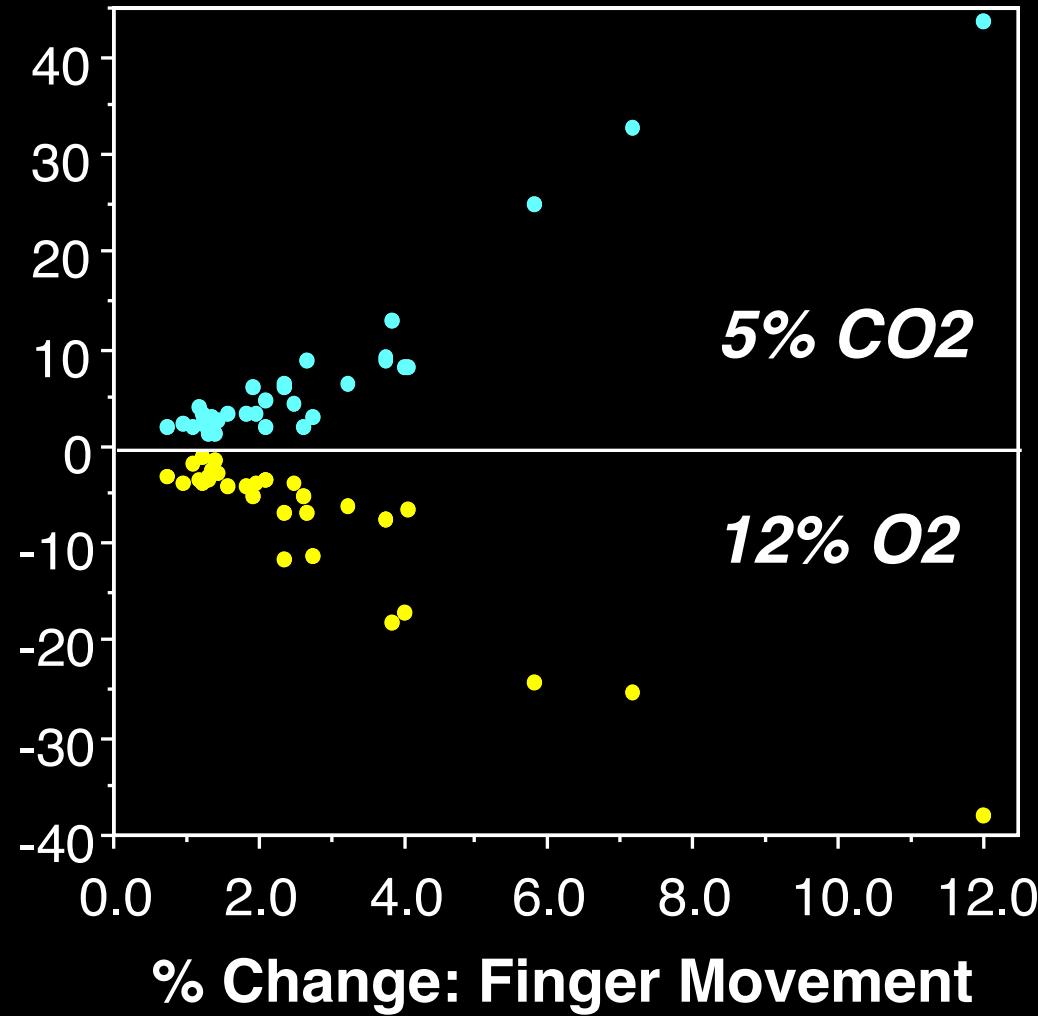


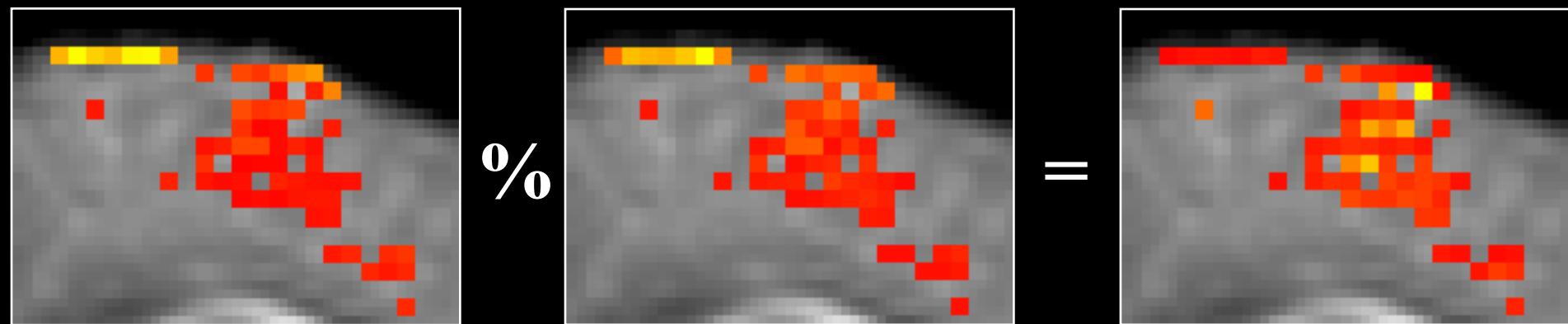
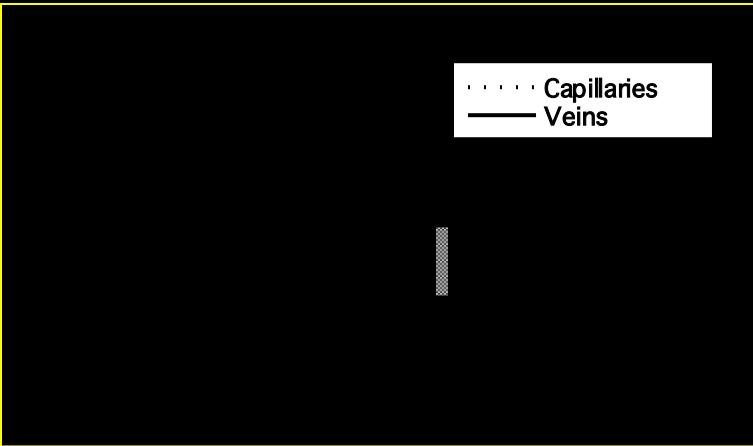
Finger
Movement

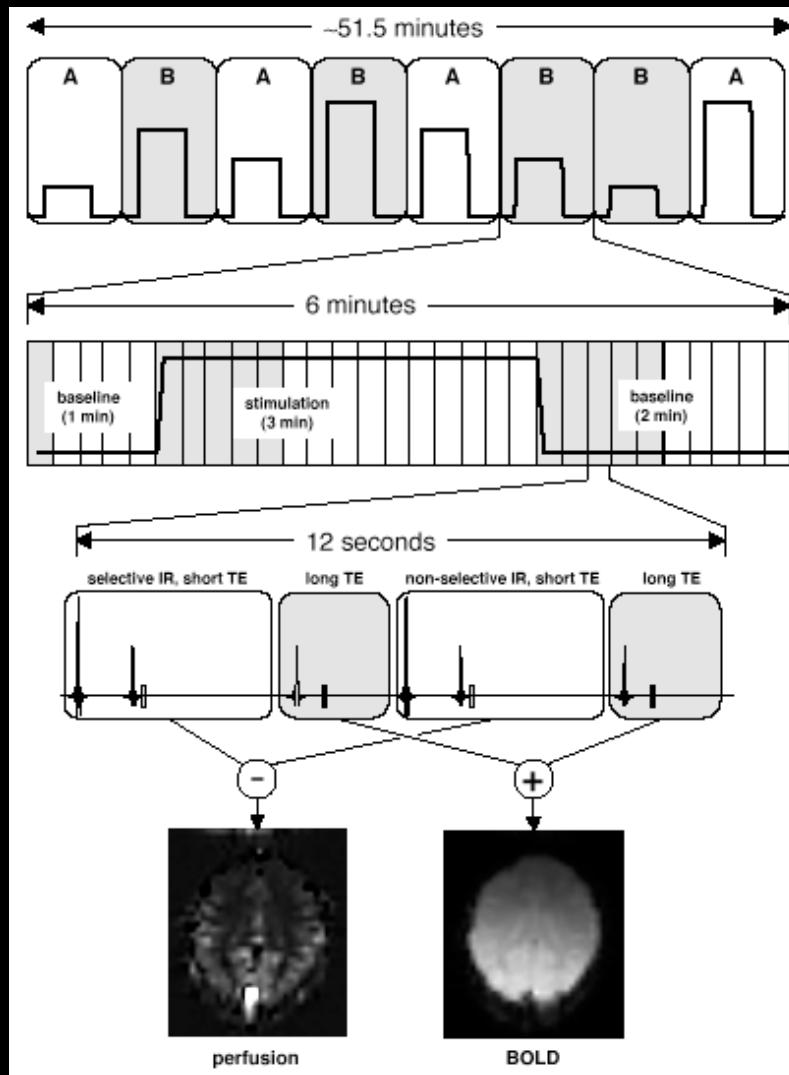
5% CO₂



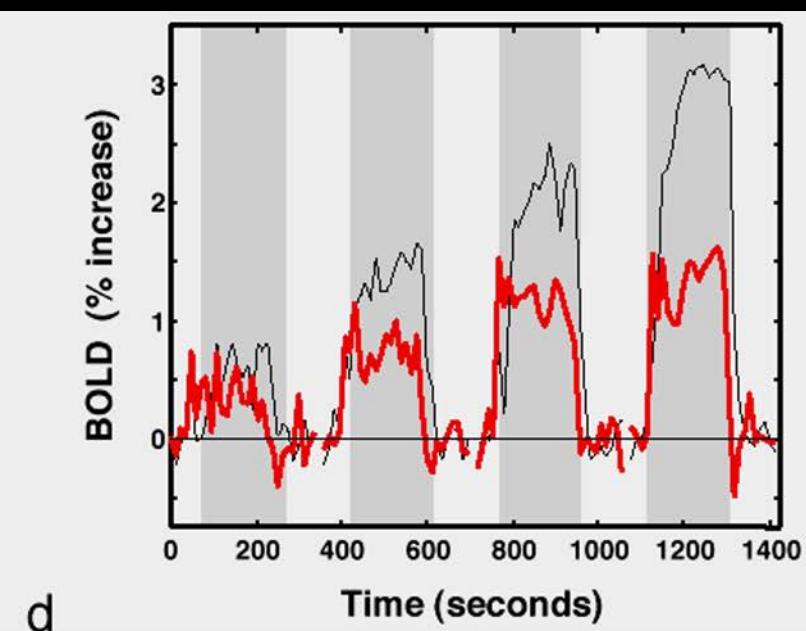
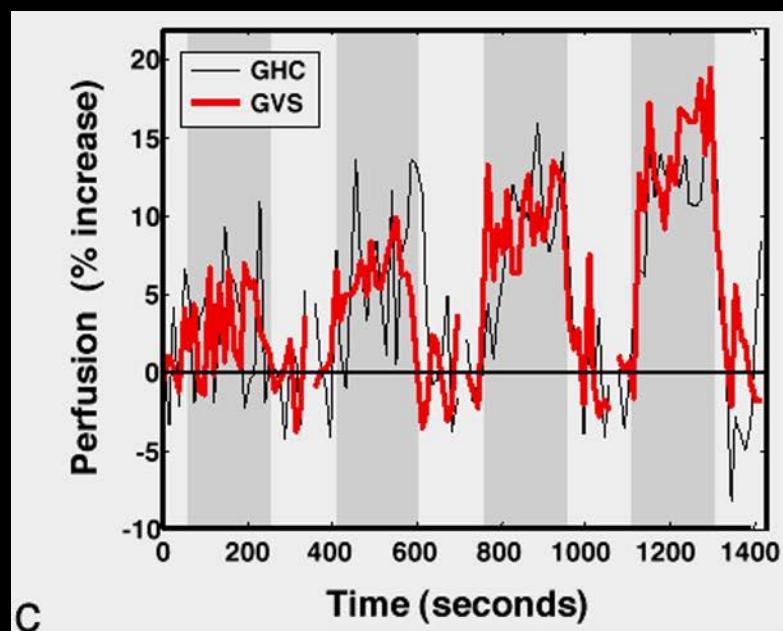
Resting State Blood Volume Weighting





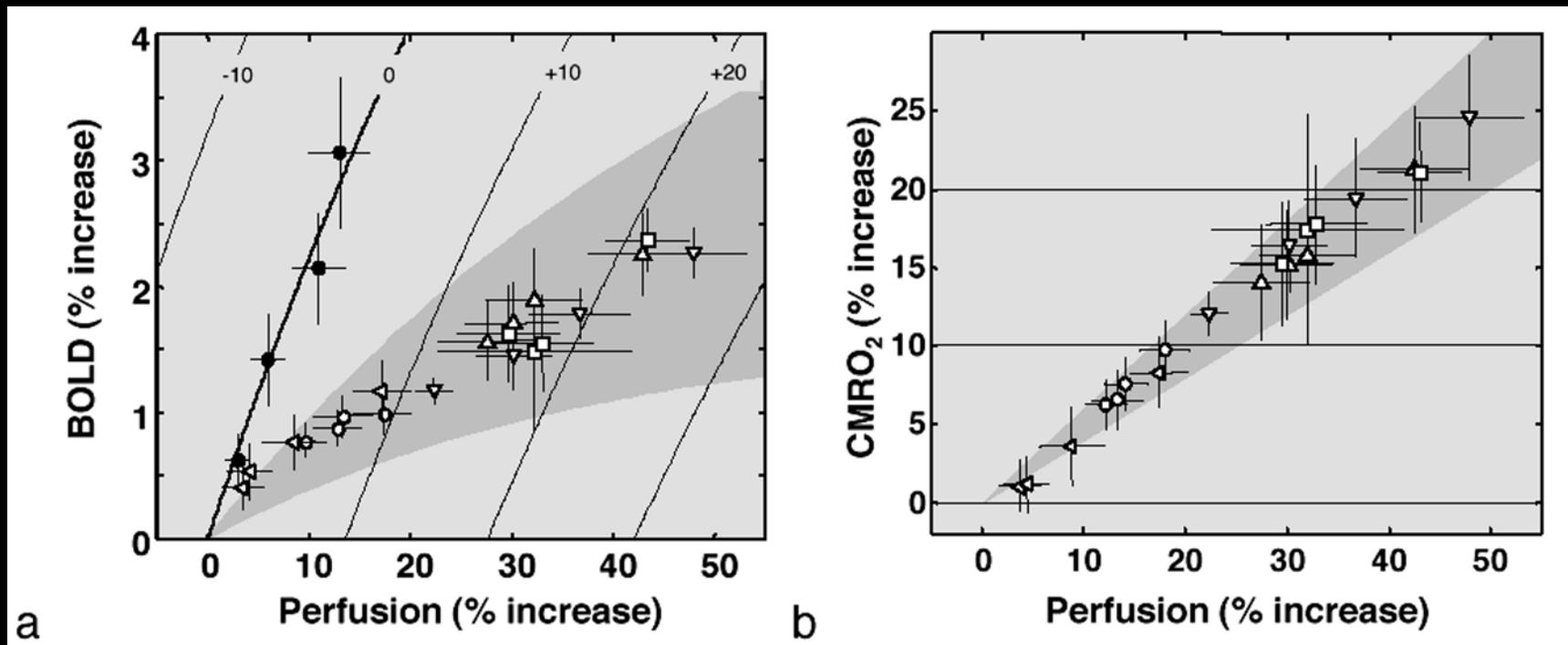


Hoge et al



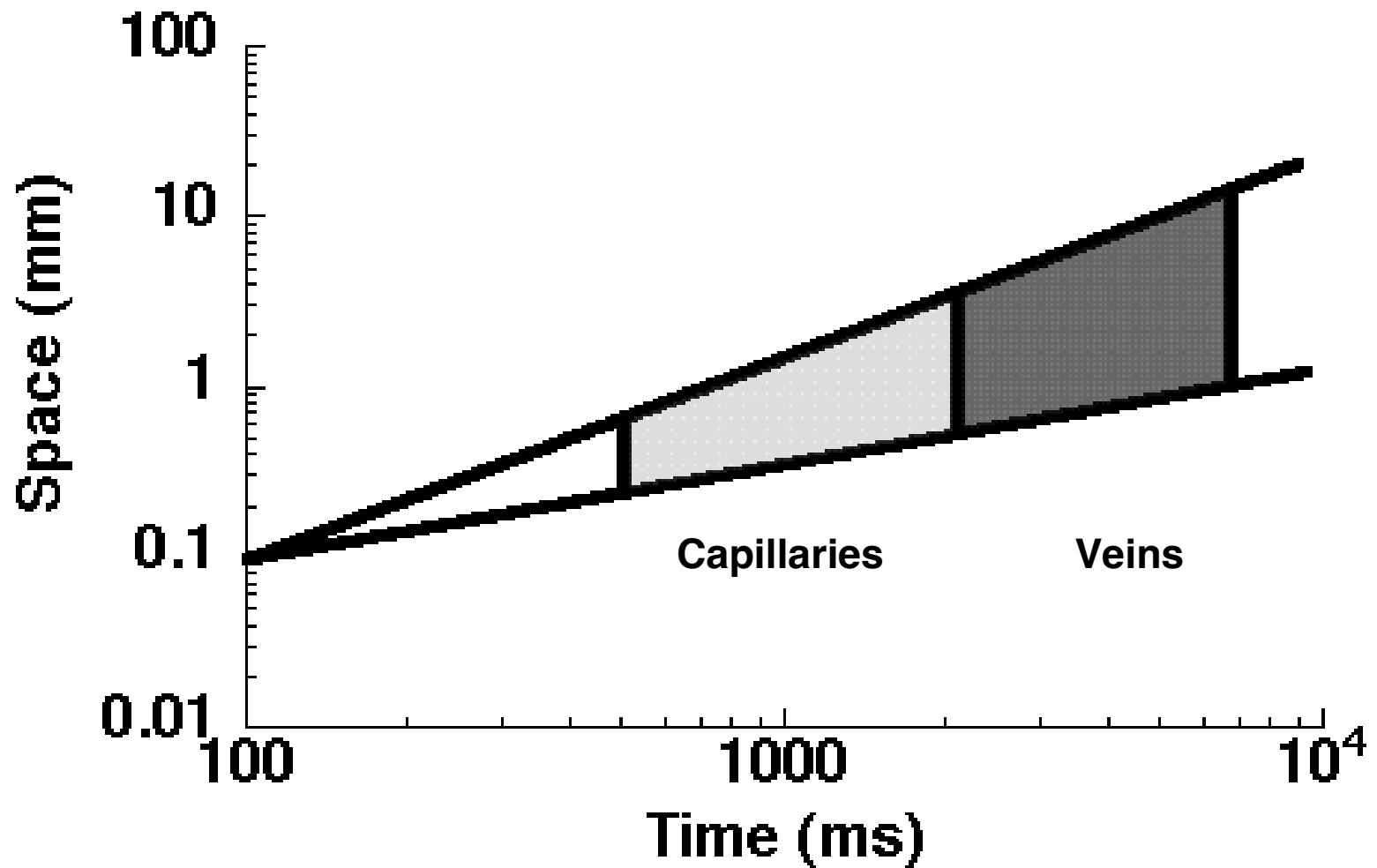
Hoge et al

Mapping CMRO₂ using CO₂ Calibration



Hoge et al

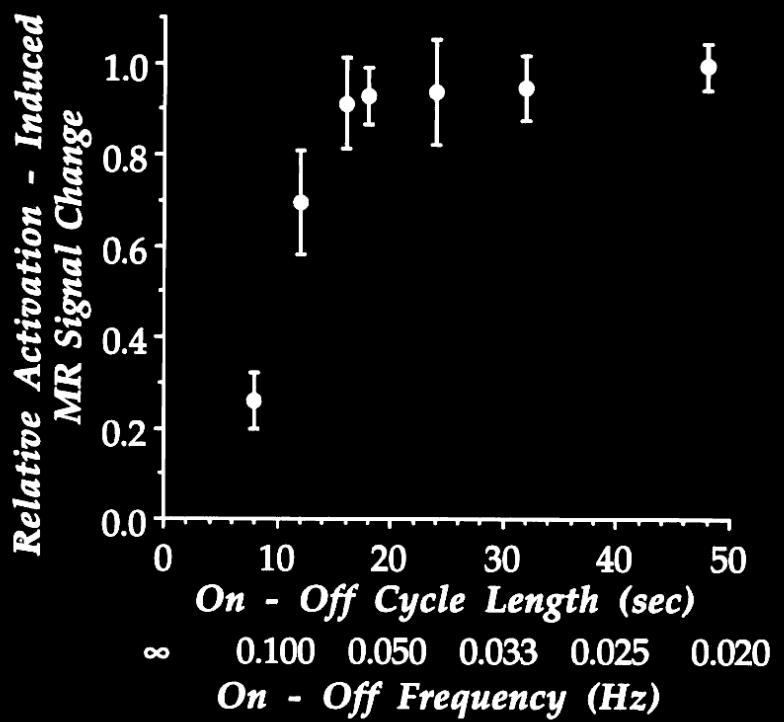
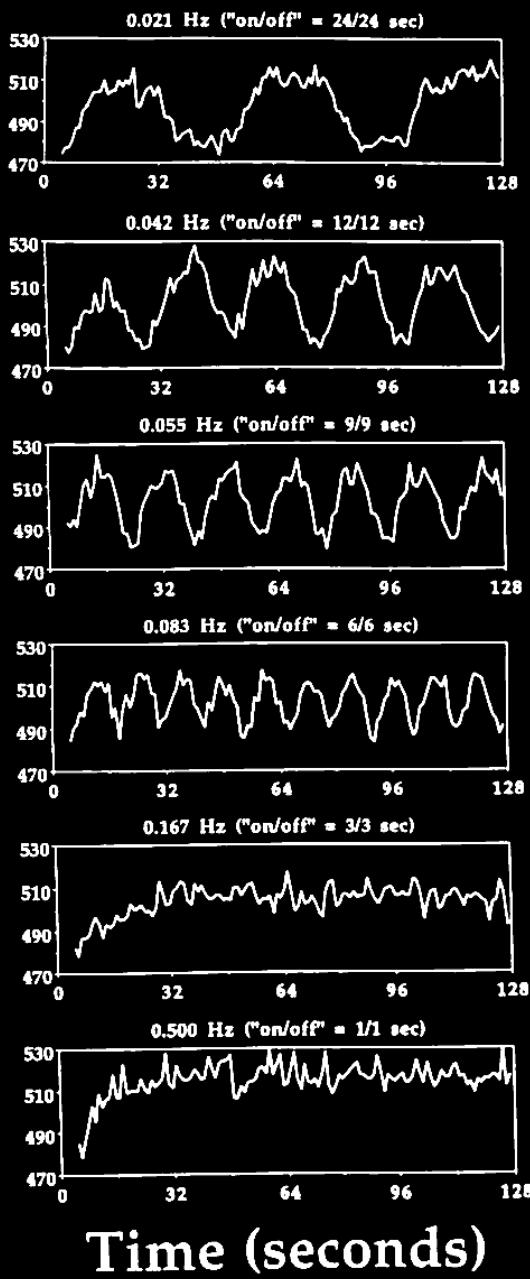
Hemodynamic Latency and Variability Following Neuronal Activation



Types of Temporal Resolution

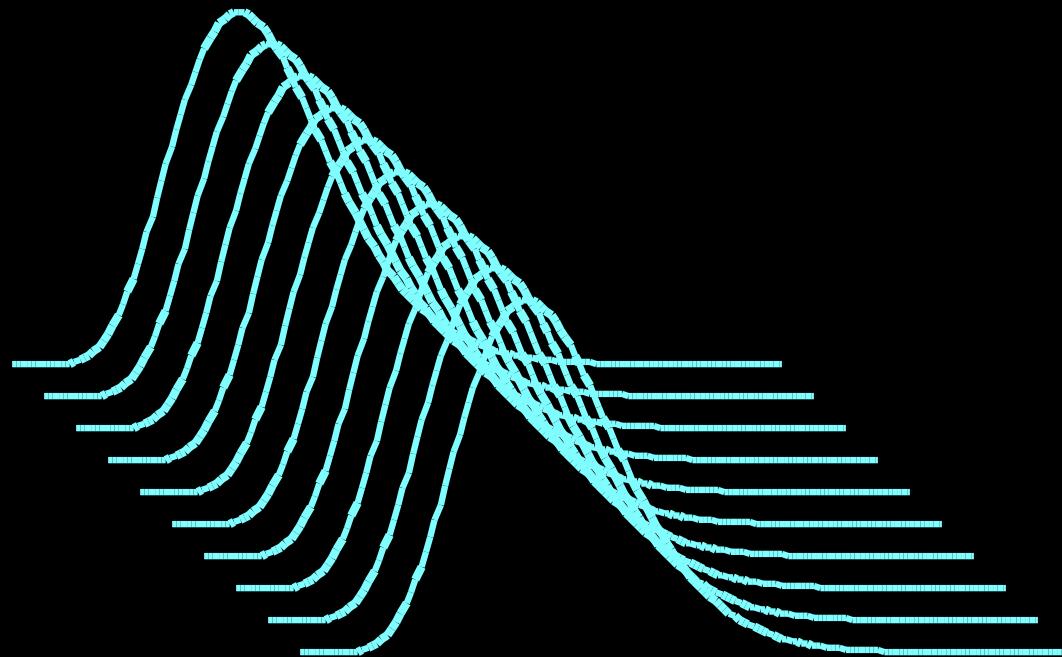
1. Maximum on-off switching rate.
2. Minimum detectable activation duration.
3. Minimum detectable difference in activation duration or onset in same region.
4. Minimum detectable activation interval across separate brain regions.
5. Maximum image acquisition rate.

MRI Signal

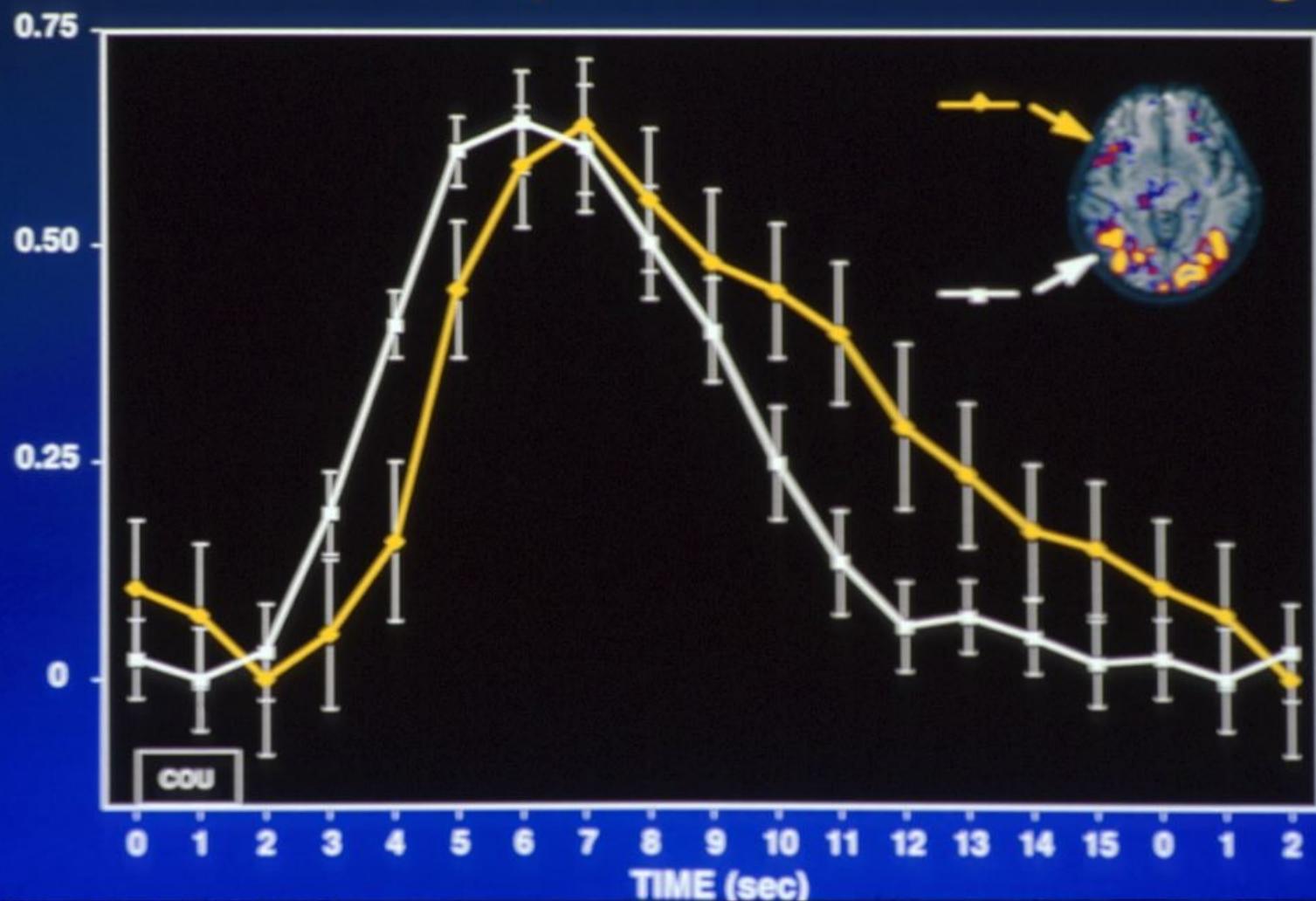


$$S = k t^{8.6} e^{-t/0.547}$$

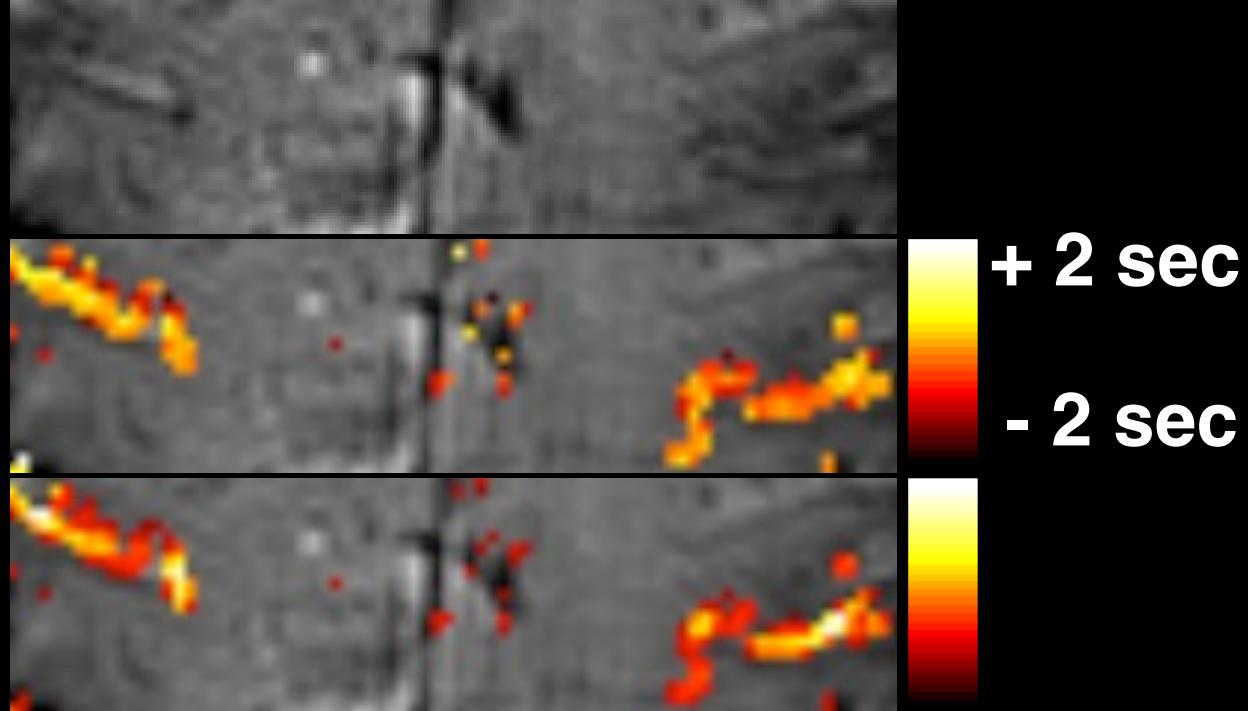
Cohen, Neuroimage 6, 93-103 (1997)



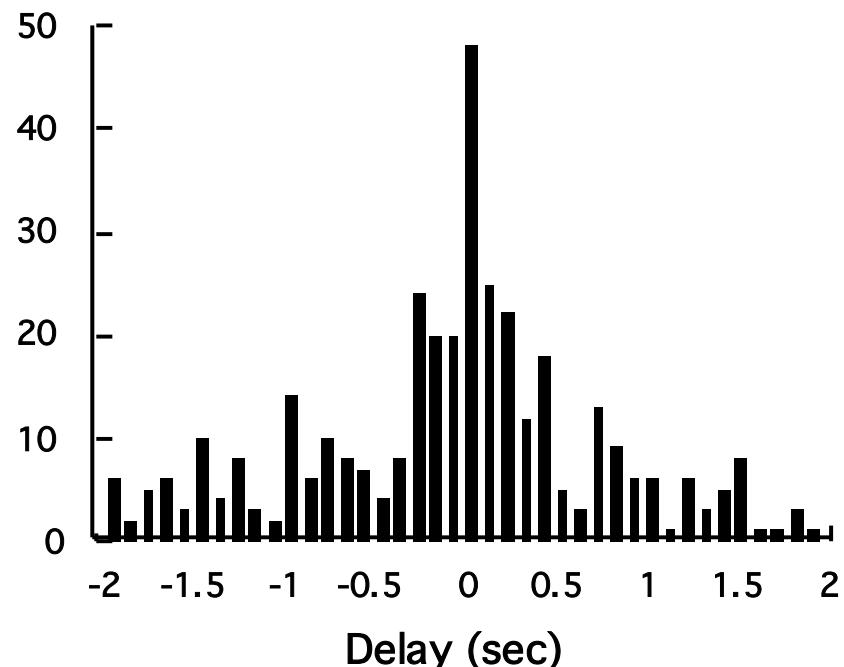
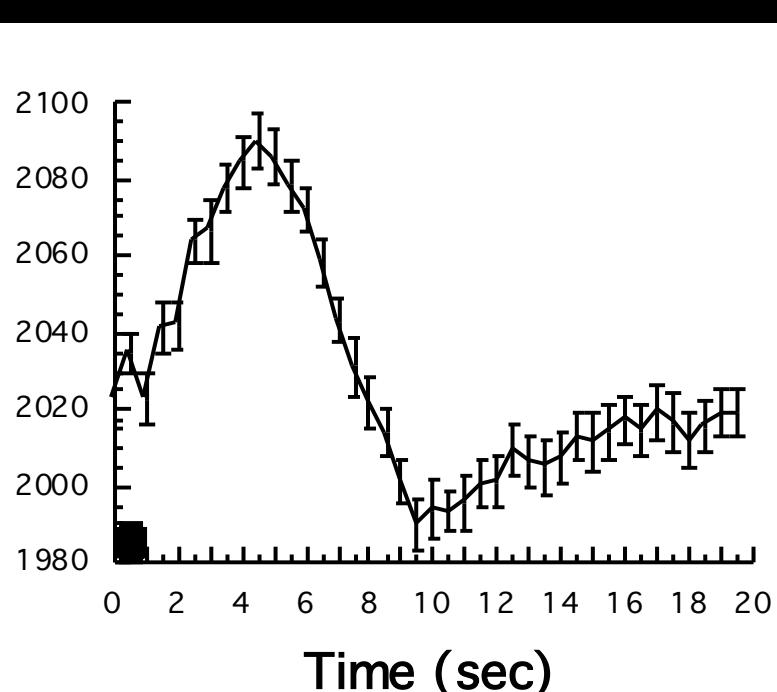
Time Course Comparison Across Brain Regions



Latency

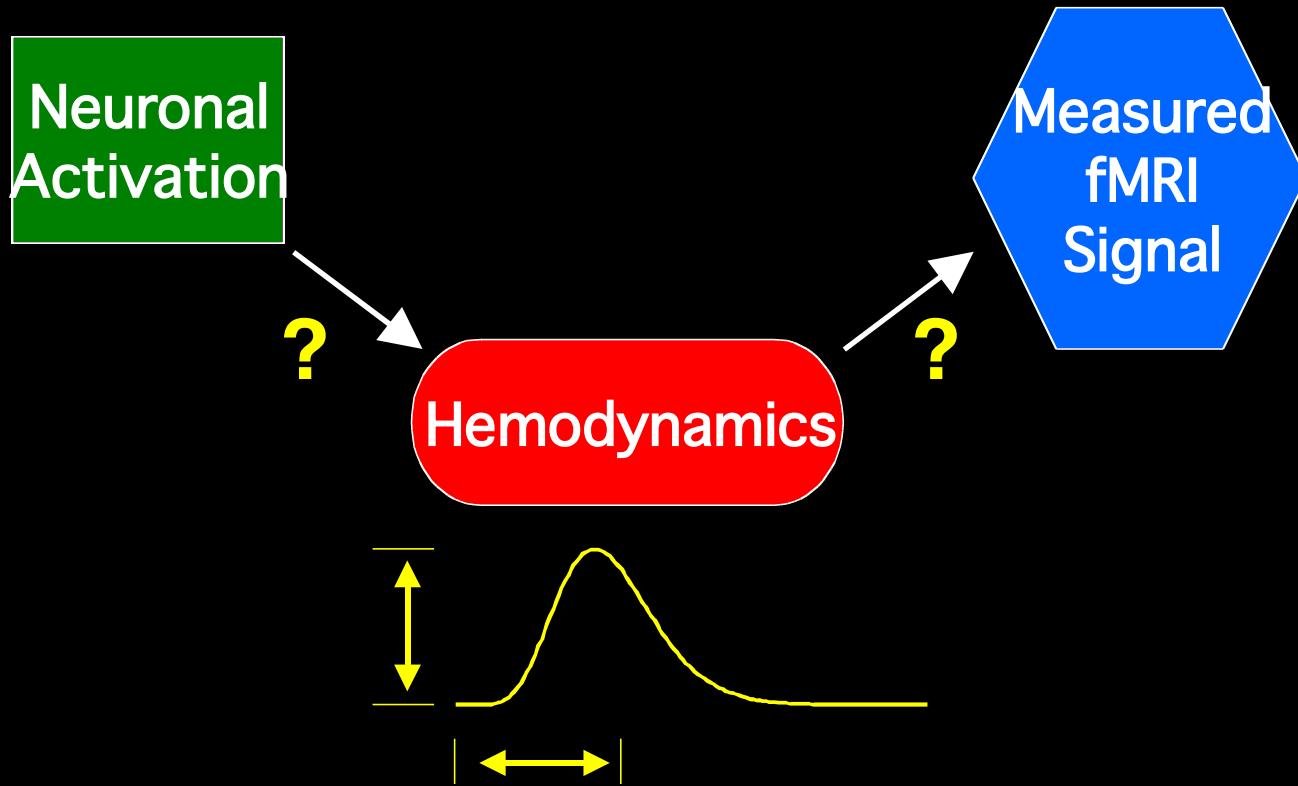


Magnitude



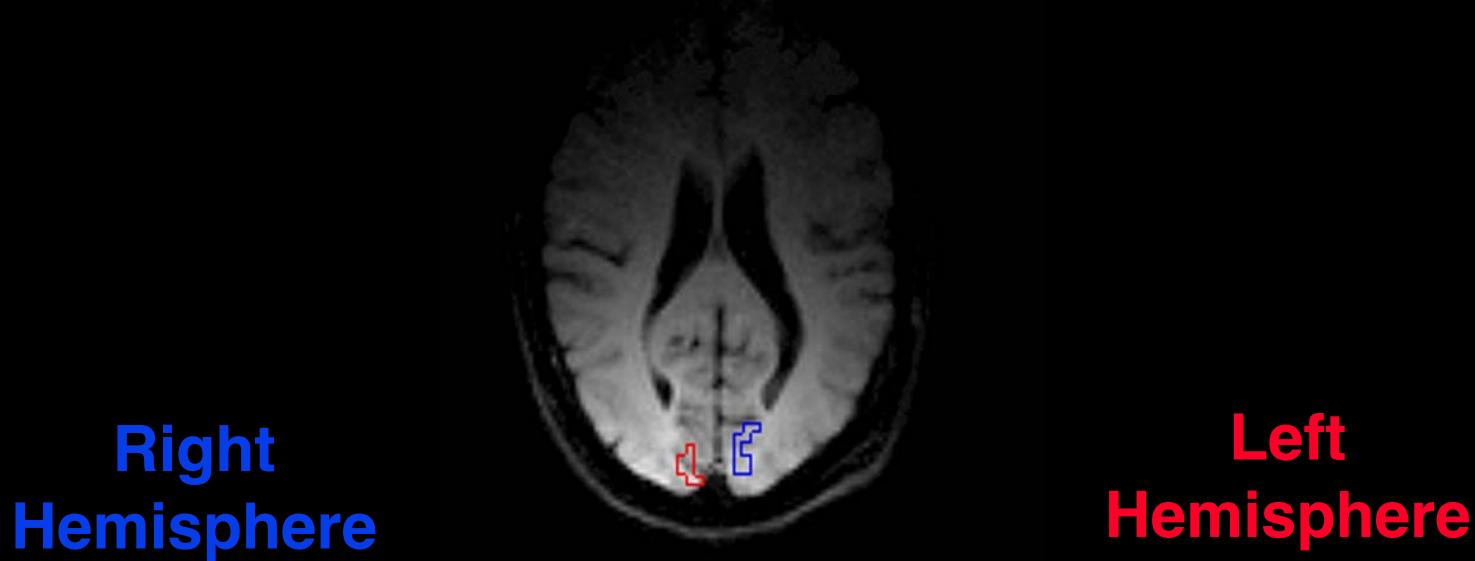
Temporal Normalization

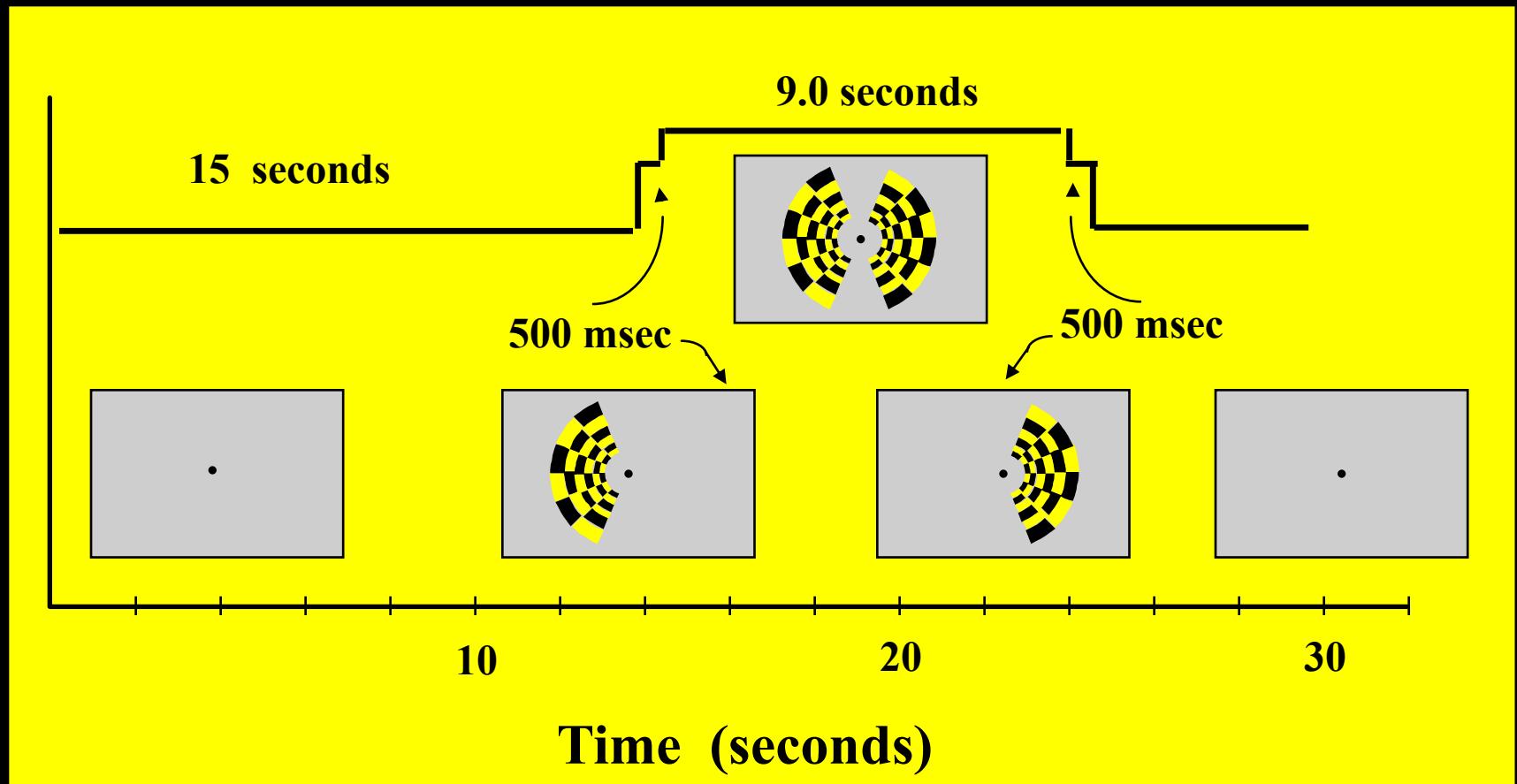
Relative Timing



Physiologic Factors

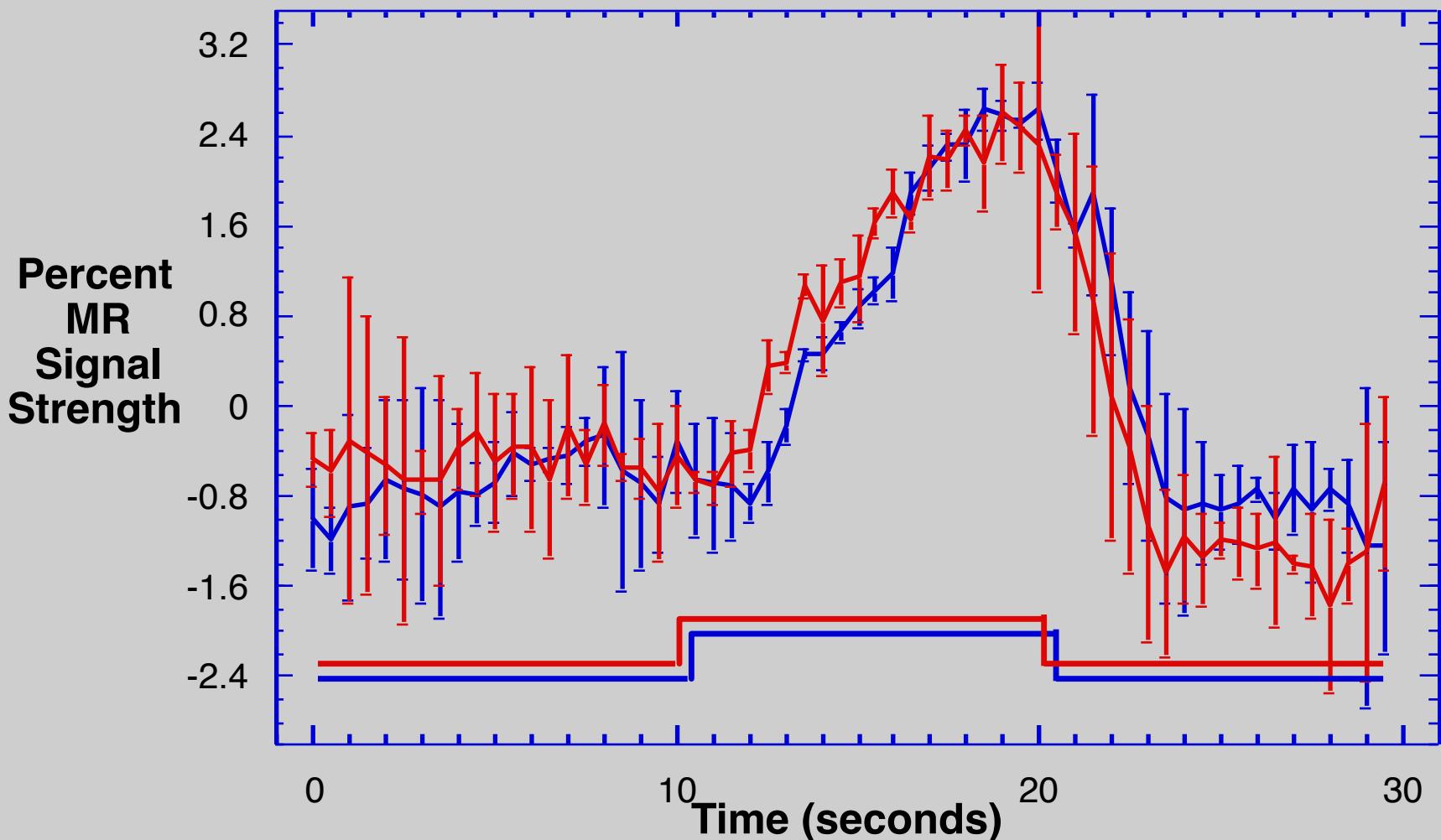
Regions of Interest Used for Hemi-Field Experiment



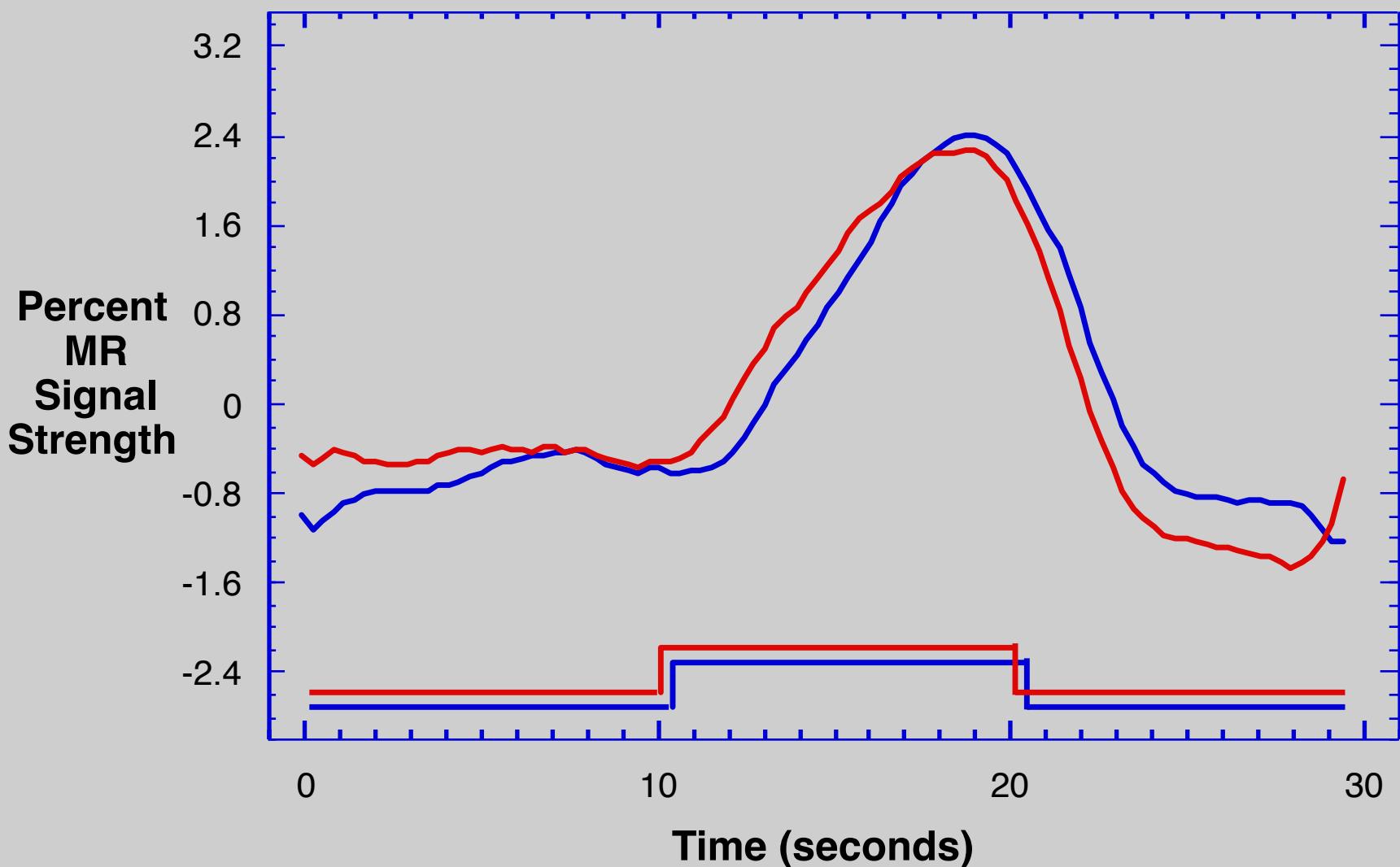


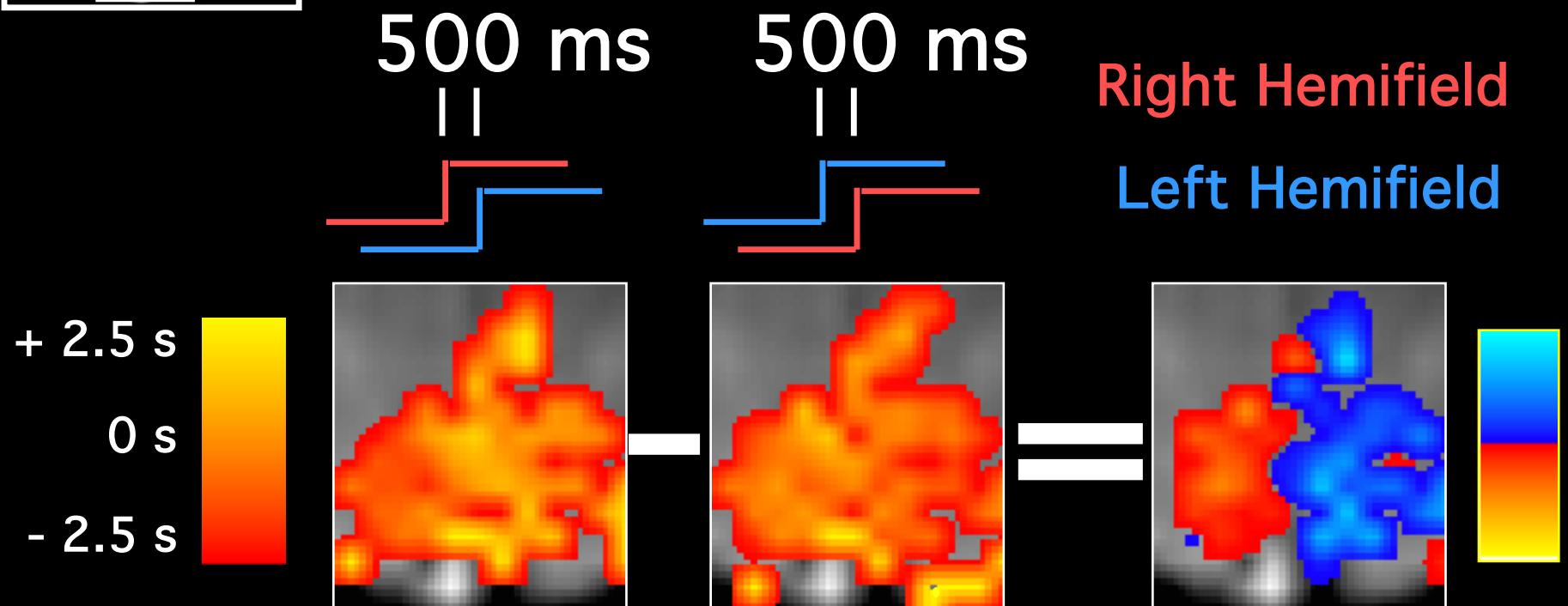
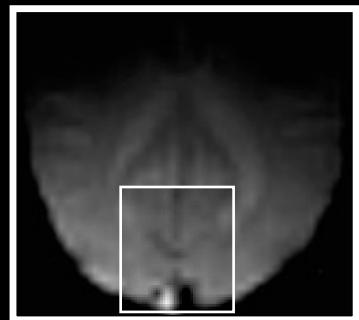
Hemi-field with 500 msec asynchrony

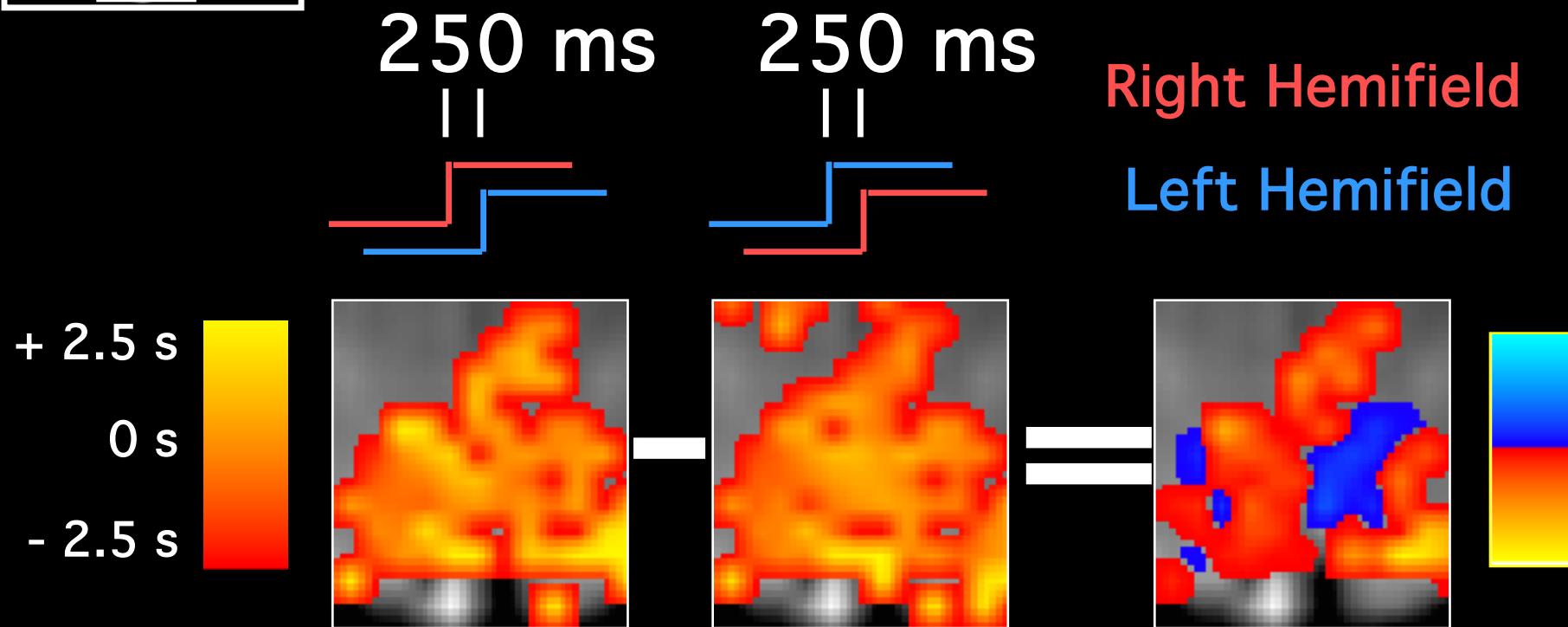
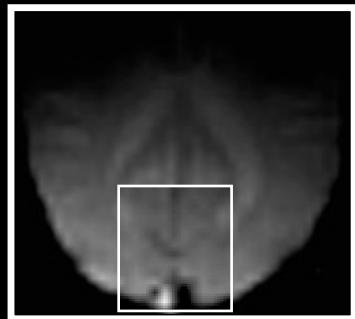
Average of 6 runs Standard Deviations Shown



Average of 6 runs Smoothed Data







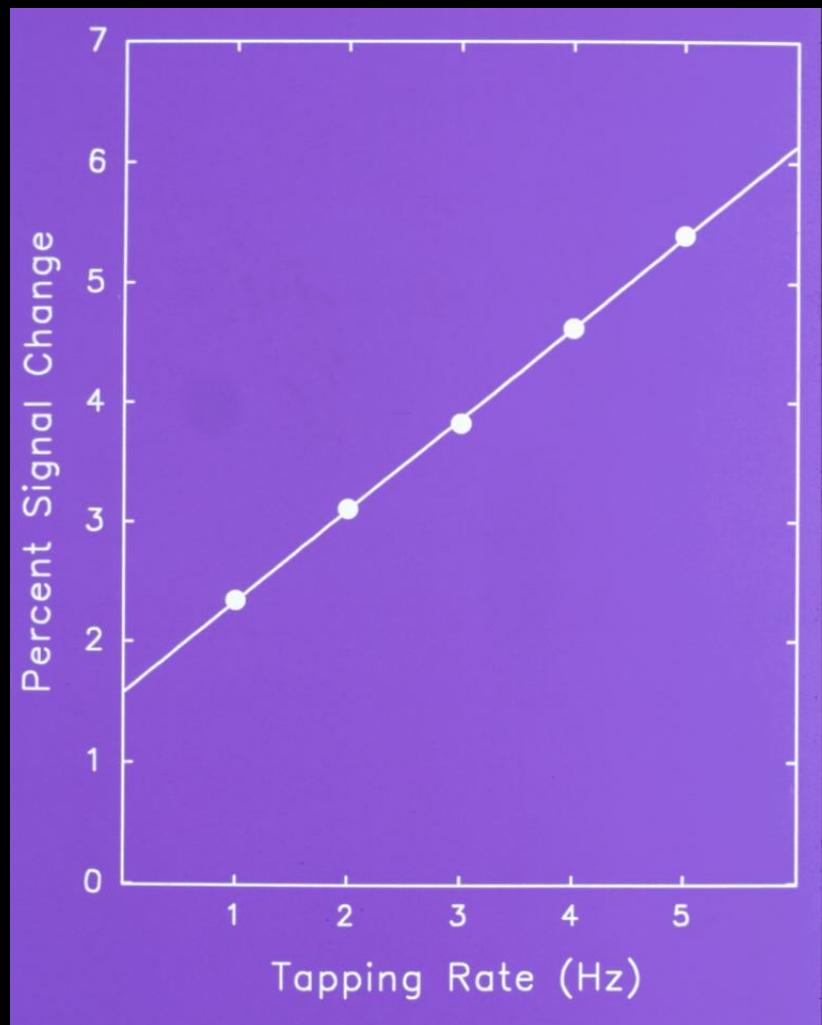
How Much?

Central Issue:

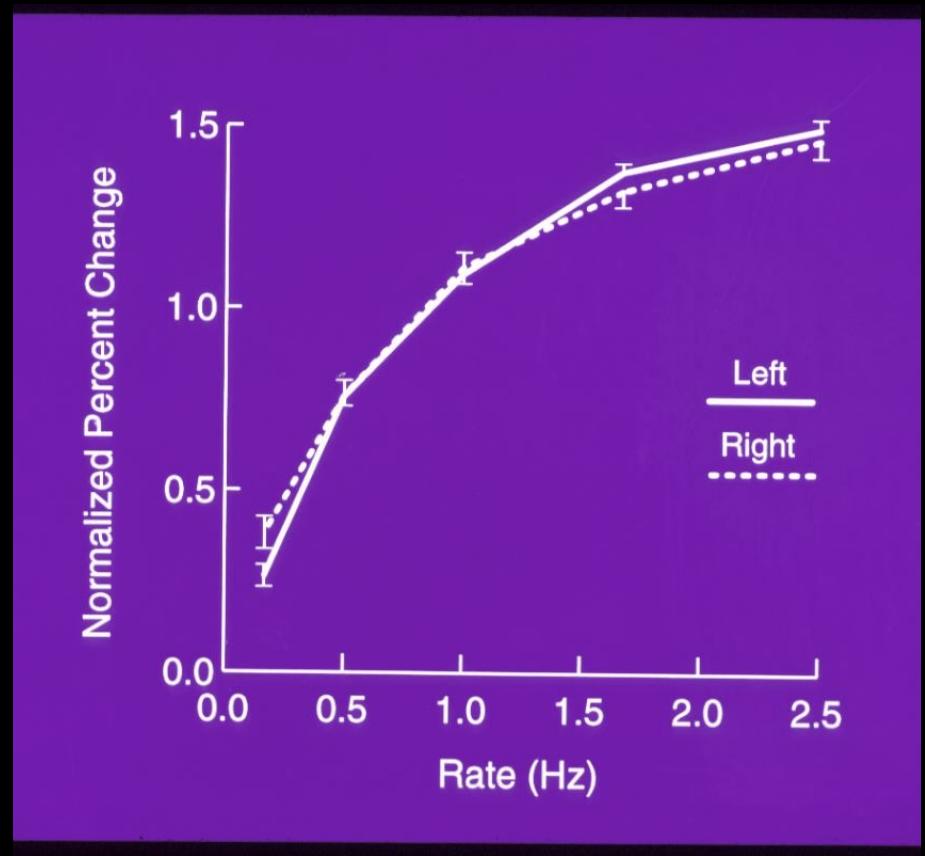
Spatial and temporal neuronal firing integration
to create an fMRI signal change.

- *is the hemodynamic response a linear system?*
- what is the dynamic range?*

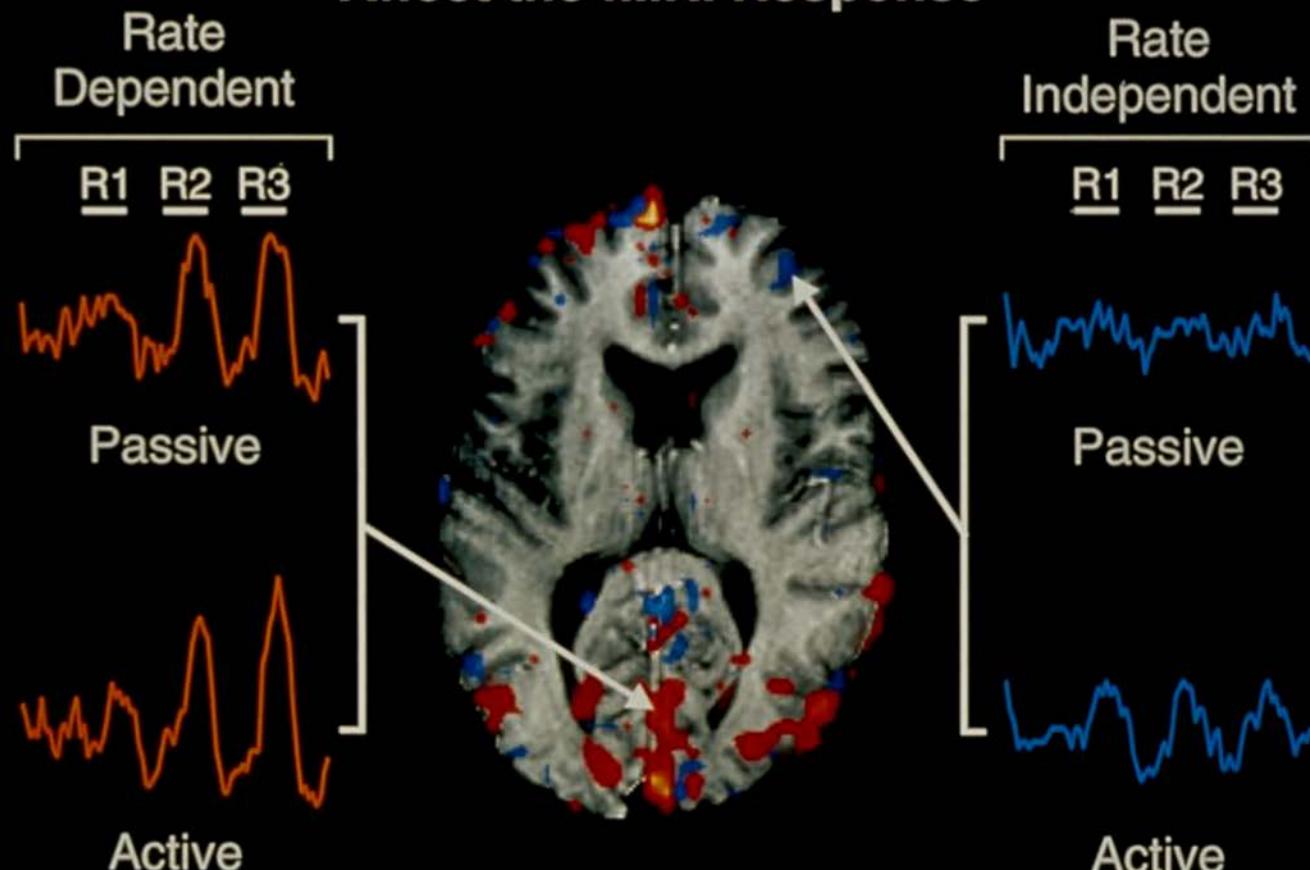
Motor Cortex



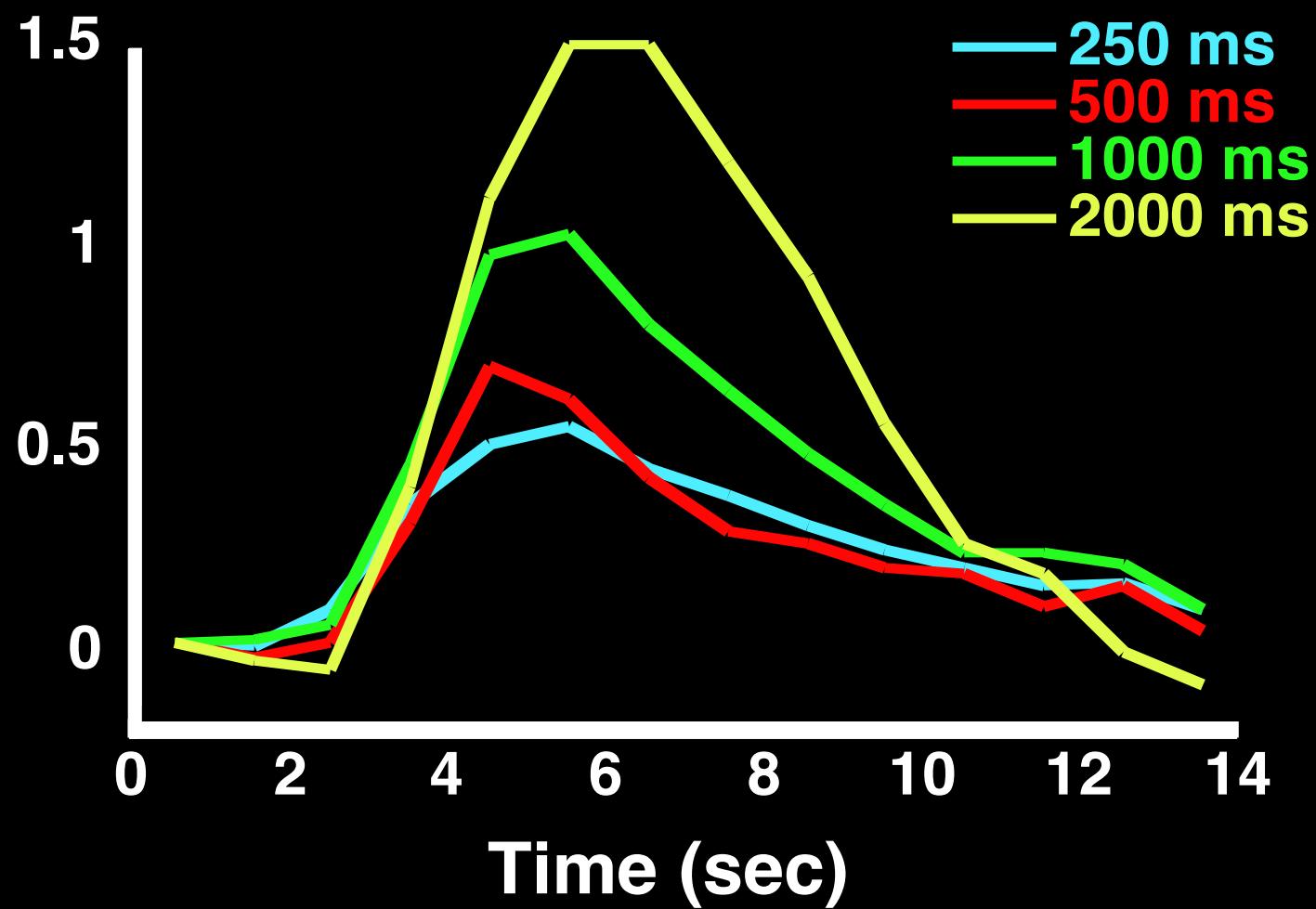
Auditory Cortex

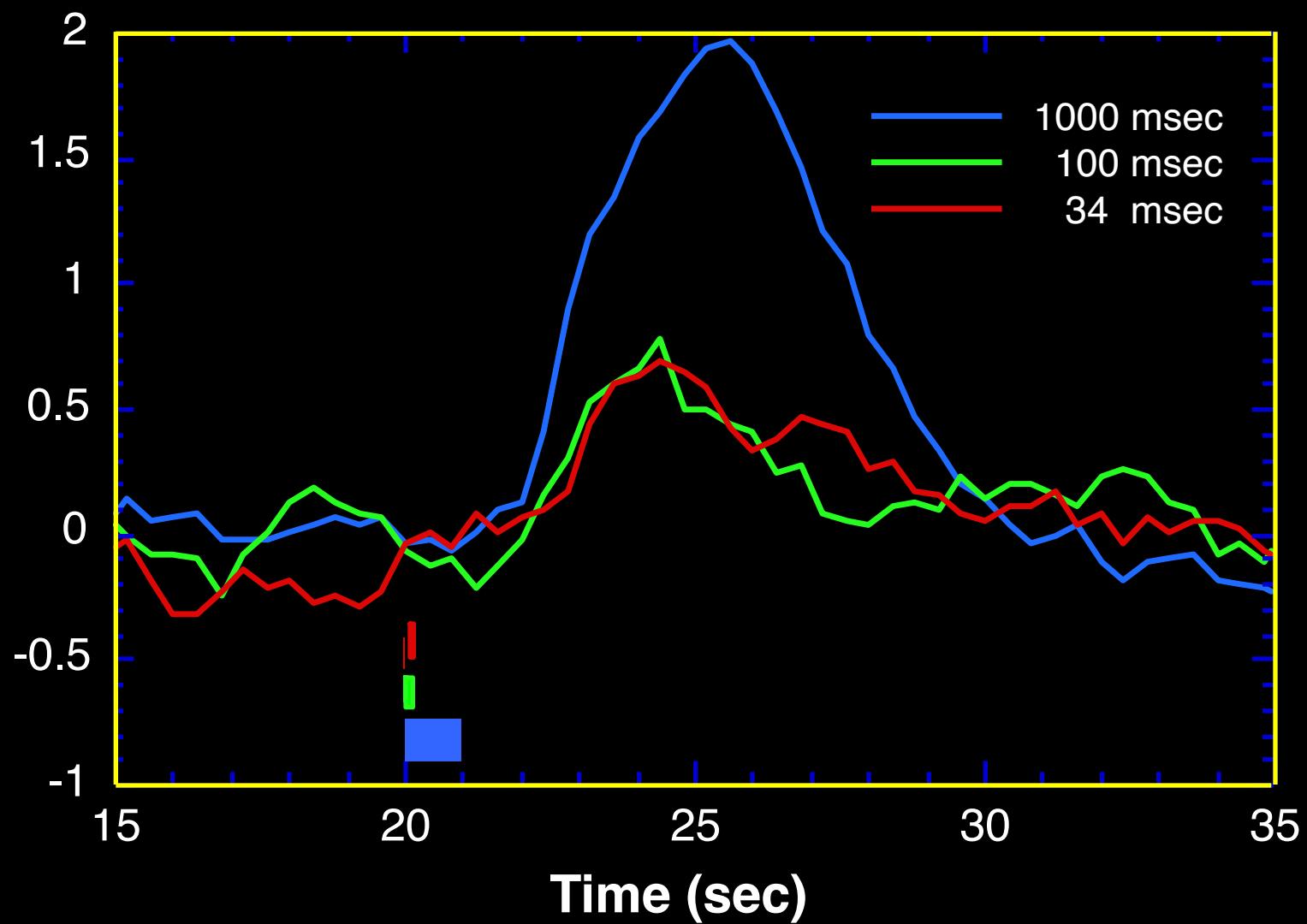


Both the Task and Presentation Rate Affect the fMRI Response

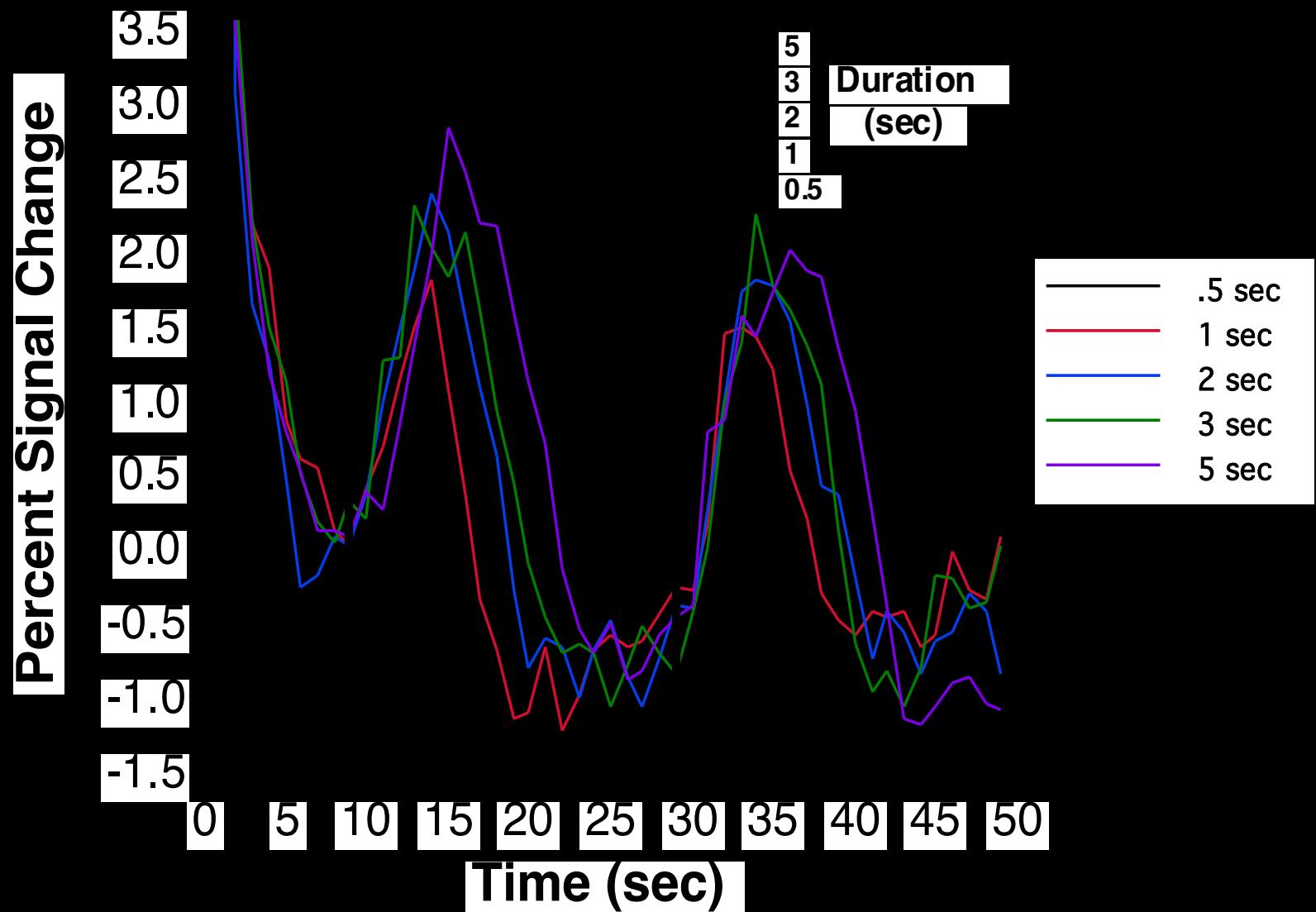


DeYoe et al.

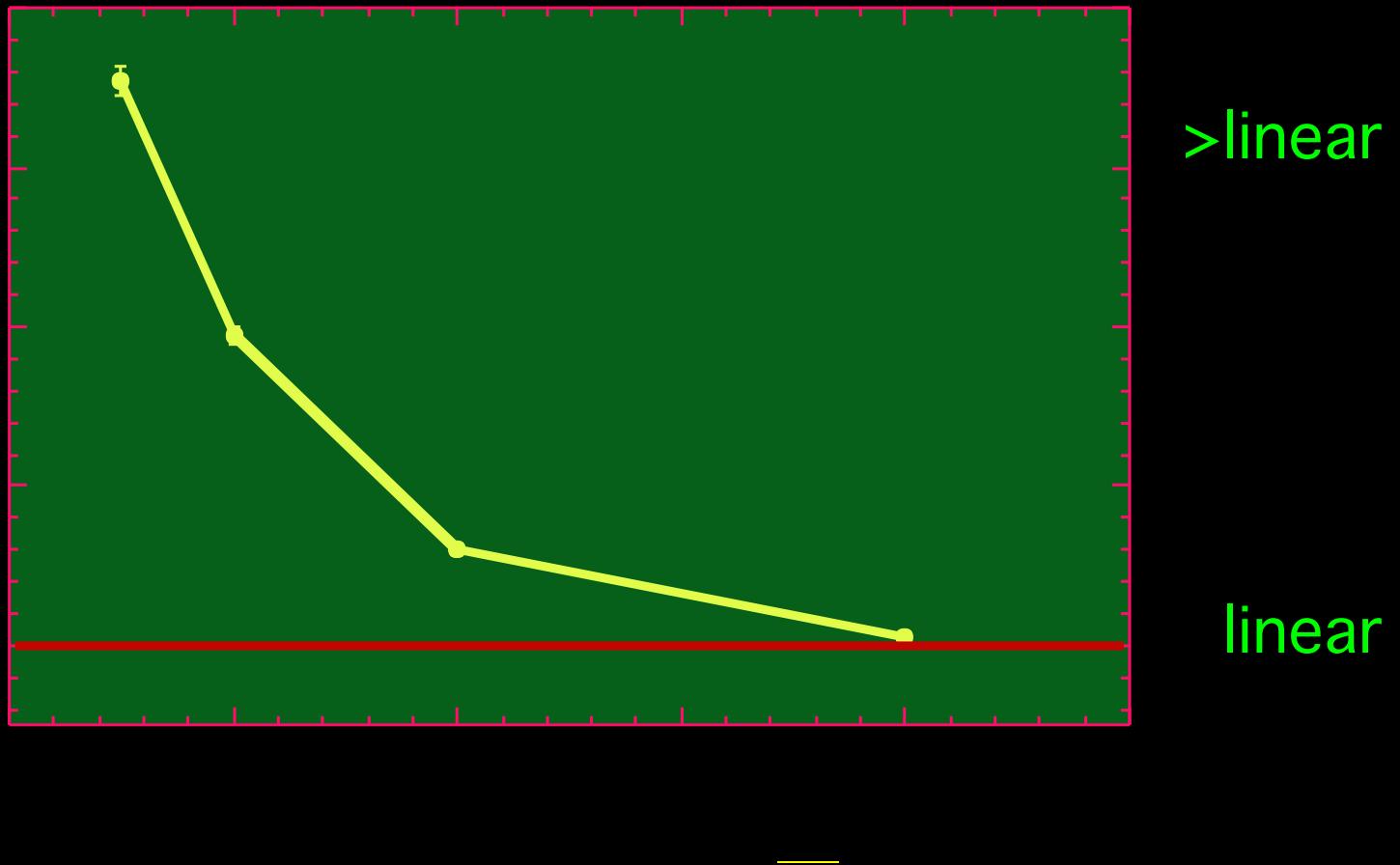




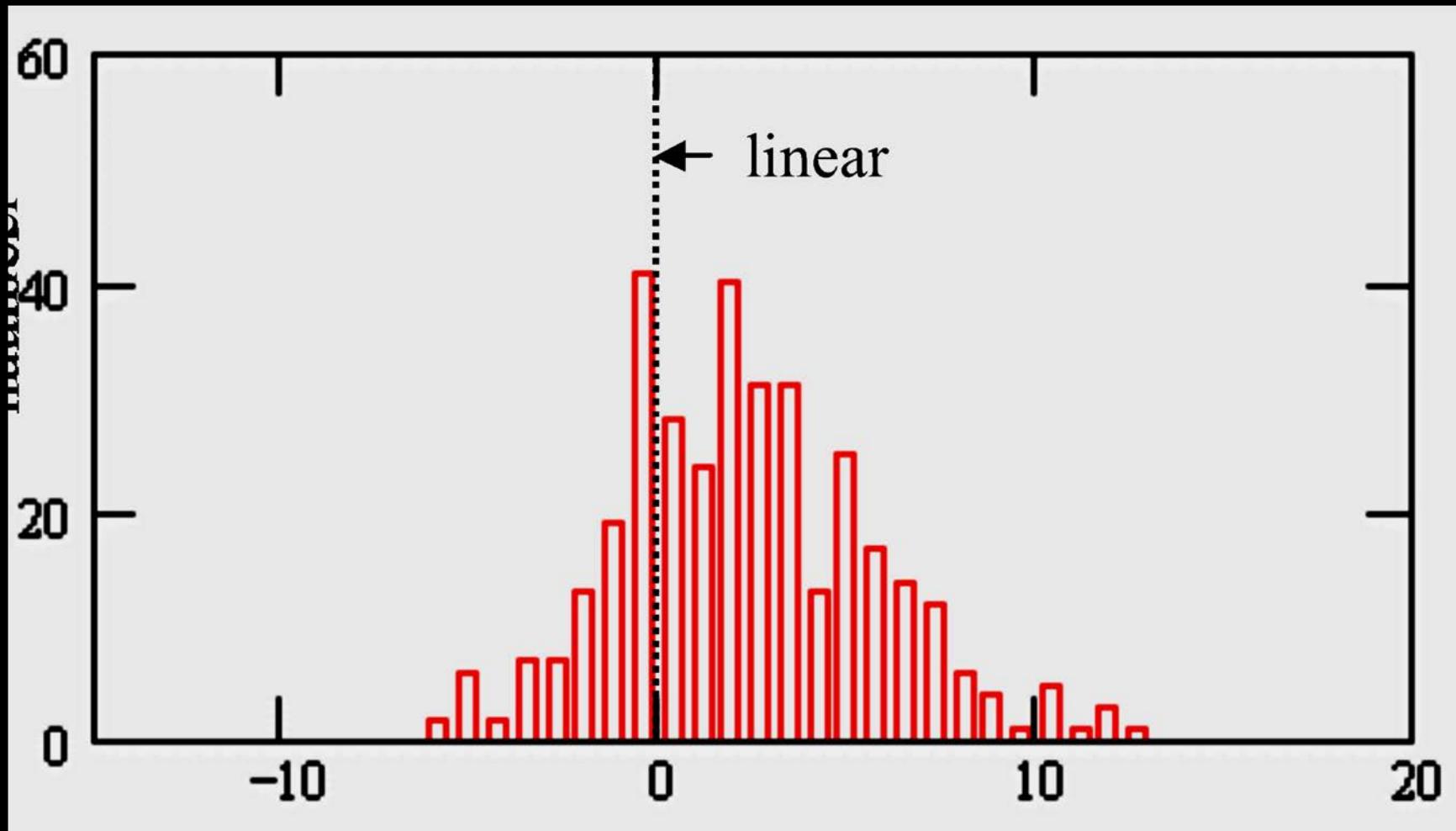
Motor Cortex



Stimulus - Duration Dependent Deviation from Linearity of the fMRI Response (Hemodynamic or Neuronal?)



Spatial Distribution of the Hemodynamic Response Linearity



Neuronal Activation Input Strategies

1. Block Design

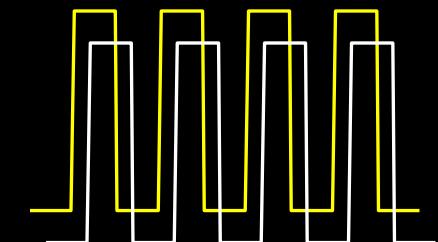
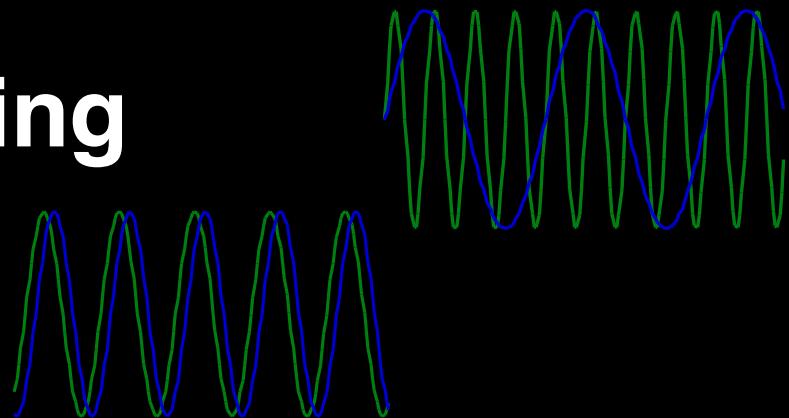
2. Frequency Encoding

3. Phase Encoding

4. Single Event

5. Orthogonal Block Design

6. Free behavior Design.



Ultimate Limits?

Spatial: 0.5 mm

Temporal: 100 ms

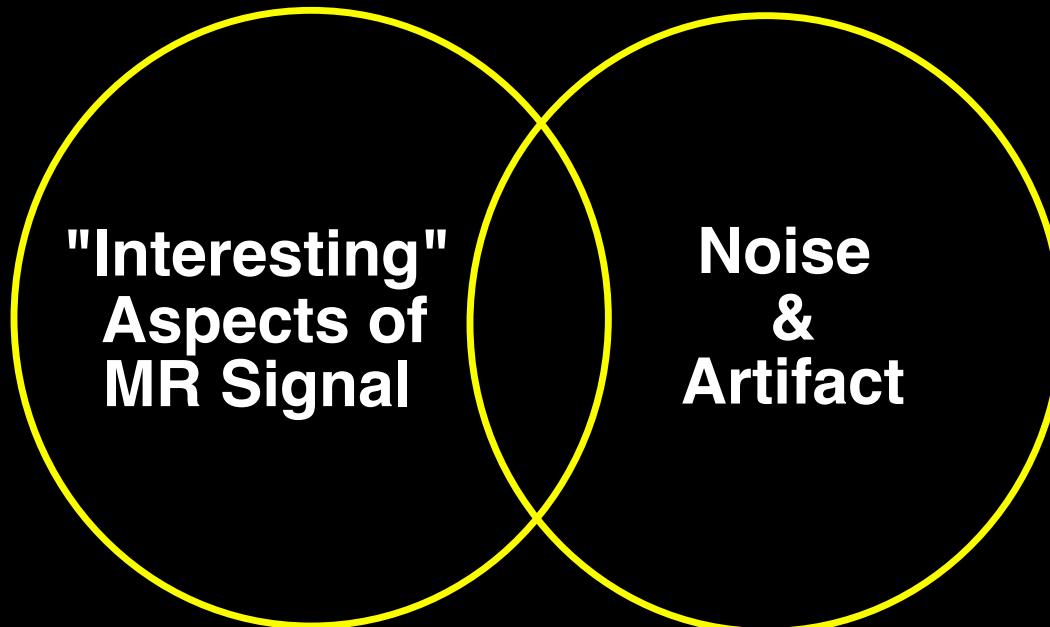
Interpretability...too early to tell, but hopeful

Neuronal Input Strategies

Peter A. Bandettini, Ph.D

Unit on Functional Imaging Methods
Laboratory of Brain and Cognition
National Institute of Mental Health

How to get the brain to do what we want it to do in the context of an fMRI experiment?



Neuronal Activation Input Strategies

1. Block Design

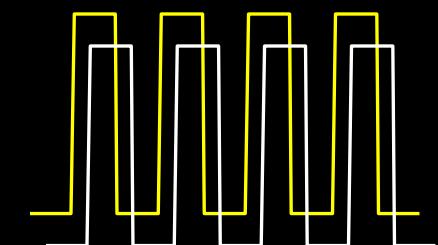
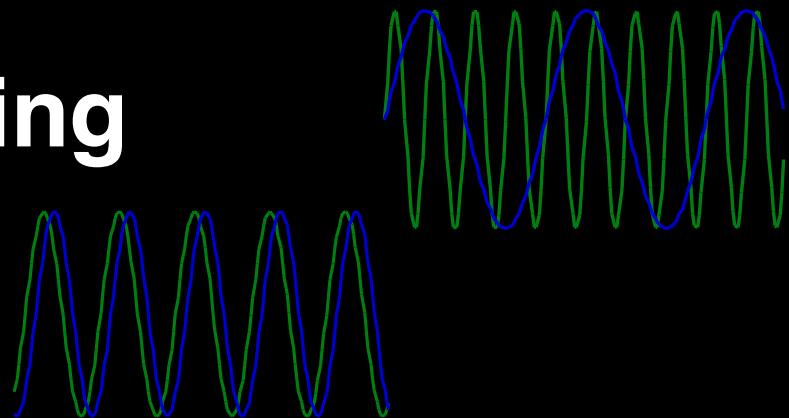
2. Frequency Encoding

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Neuronal Activation Input Strategies

1. Block Design

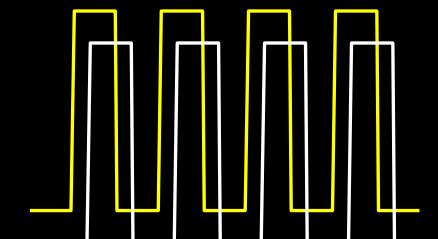
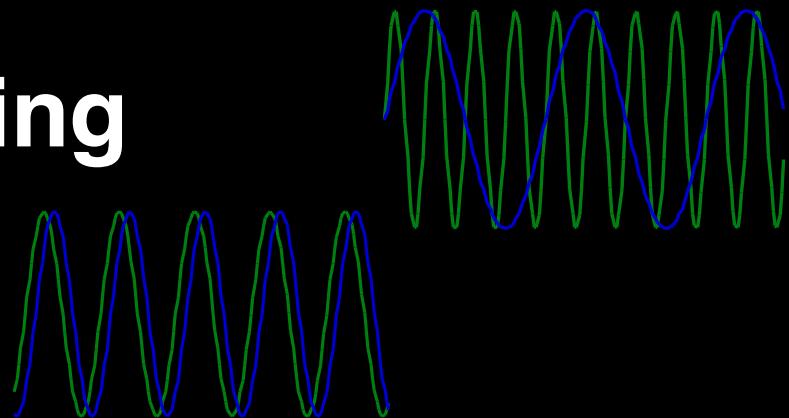
2. Frequency Encoding

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4. Single Event

5. Orthogonal Block Design

6. Free behavior Design.



Neuronal Activation Input Strategies

1. Block Design

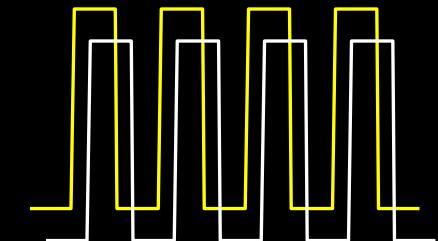
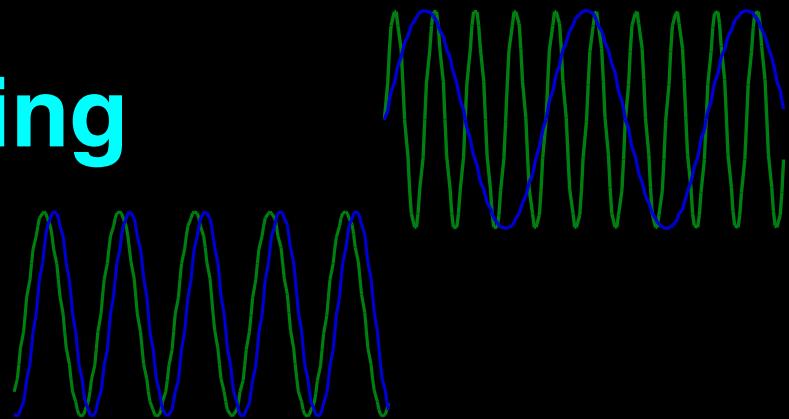
2. Frequency Encoding

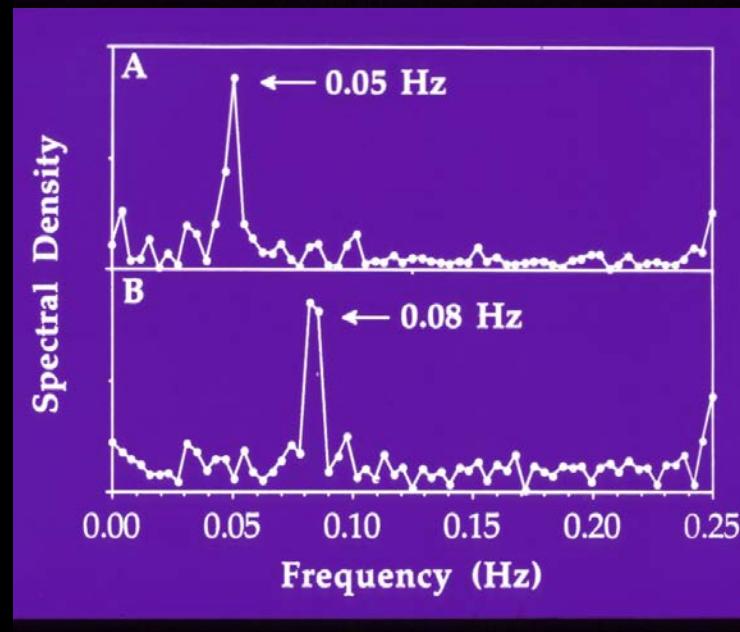
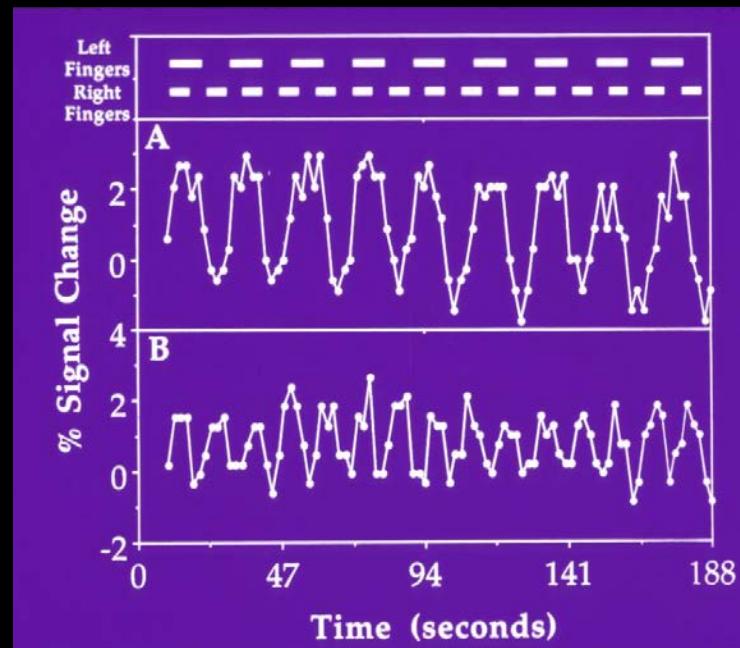
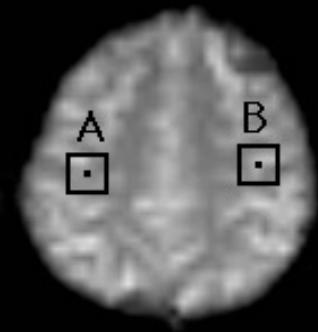
3. Phase Encoding

4. Single Event

5. Orthogonal Block Design

6. Free behavior Design.

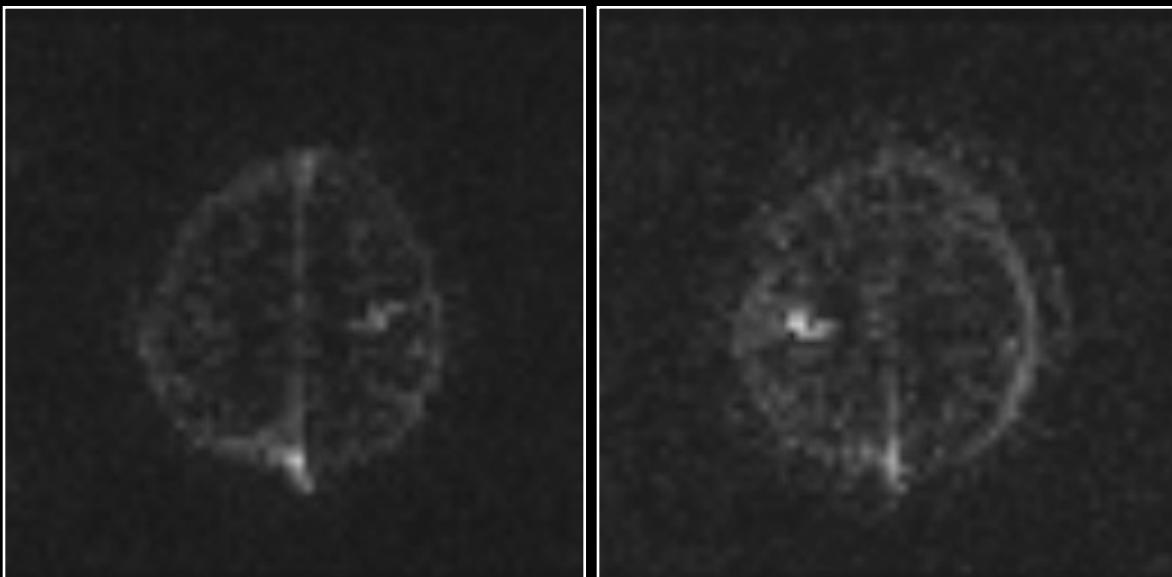




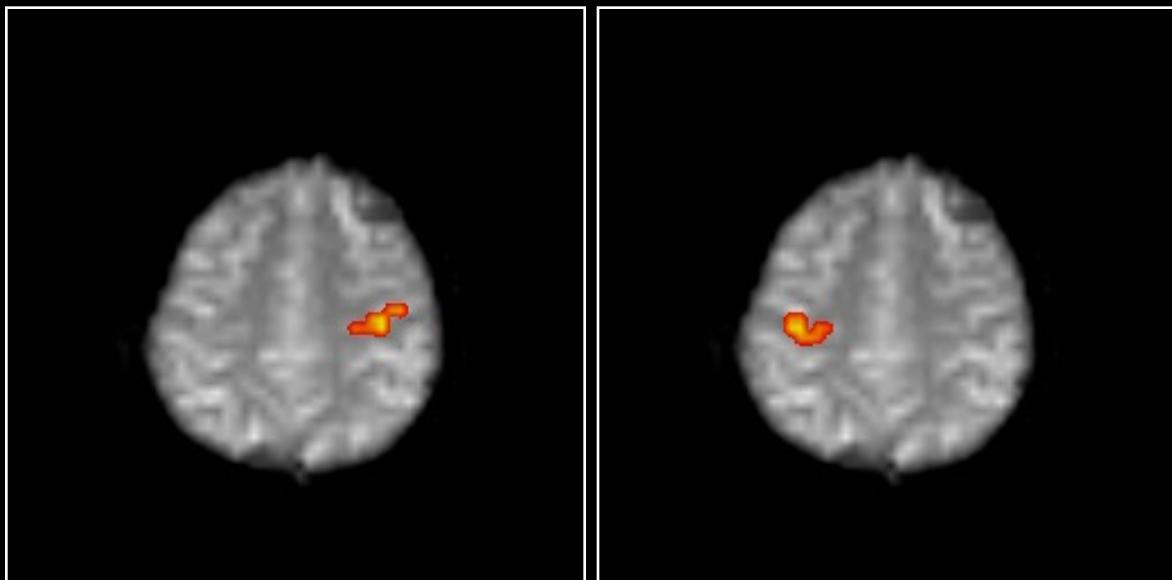
0.08 Hz

0.05 Hz

**spectral
density**



**c.c. > 0.5
with spectra**



Neuronal Activation Input Strategies

1. Block Design

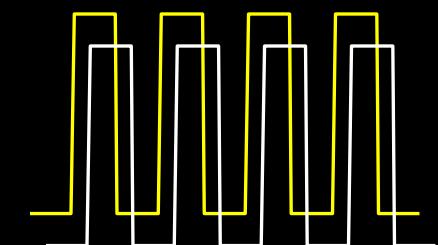
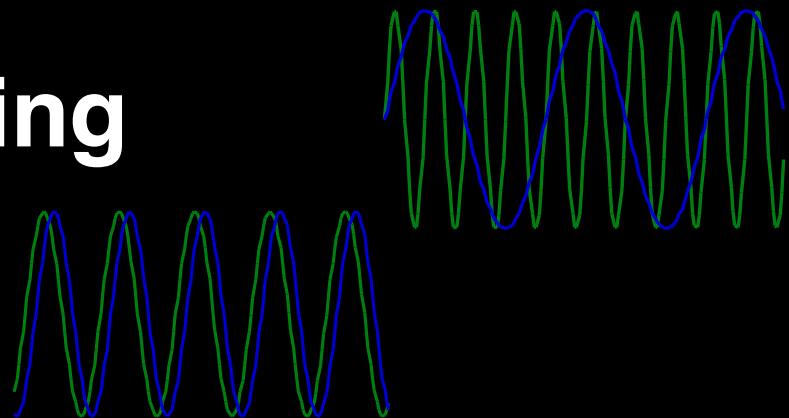
2. Frequency Encoding

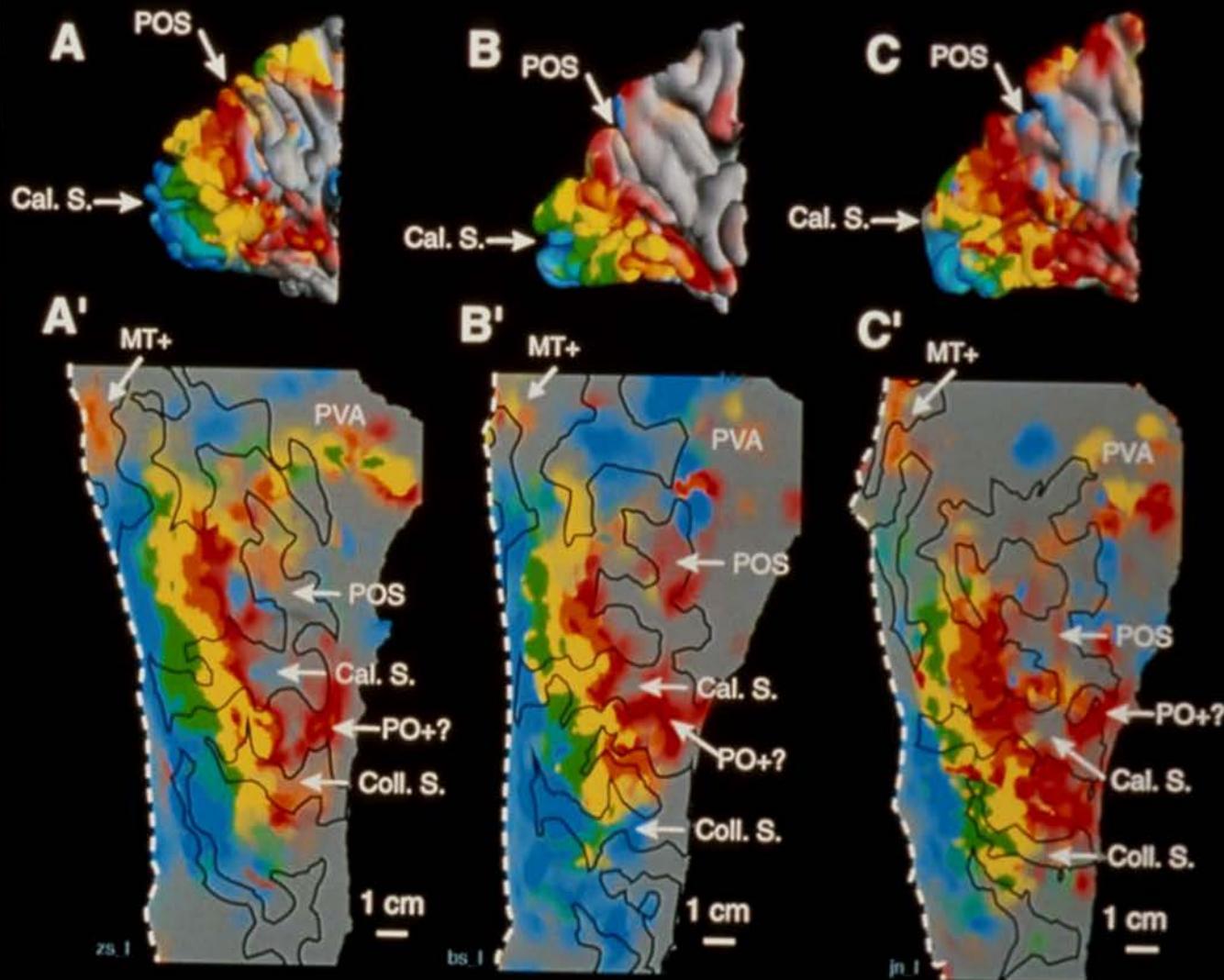
3. Phase Encoding

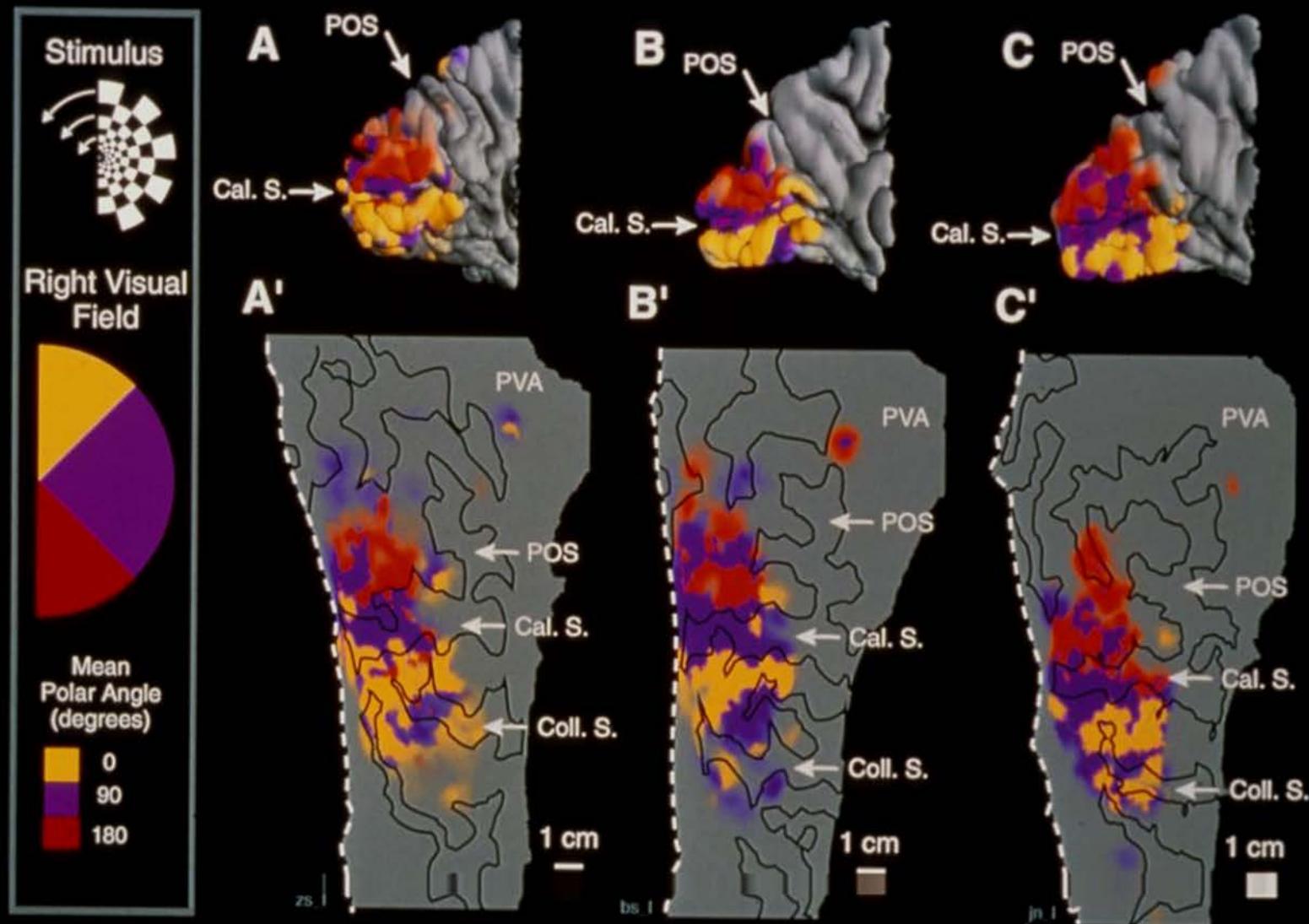
4. Single Event

5. Orthogonal Block Design

6. Free behavior Design.







Neuronal Activation Input Strategies

1. Block Design

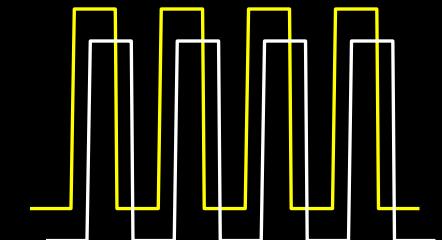
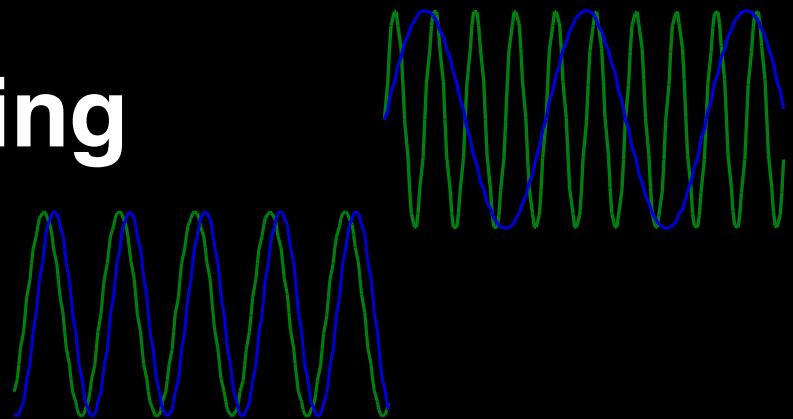
2. Frequency Encoding

3. Phase Encoding

4. Single Event

5. Orthogonal Block Design

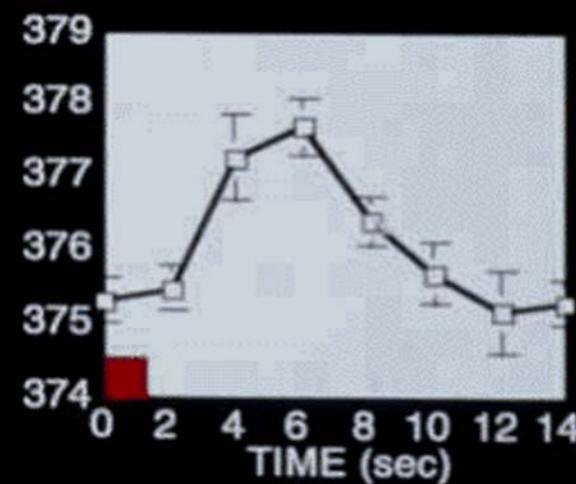
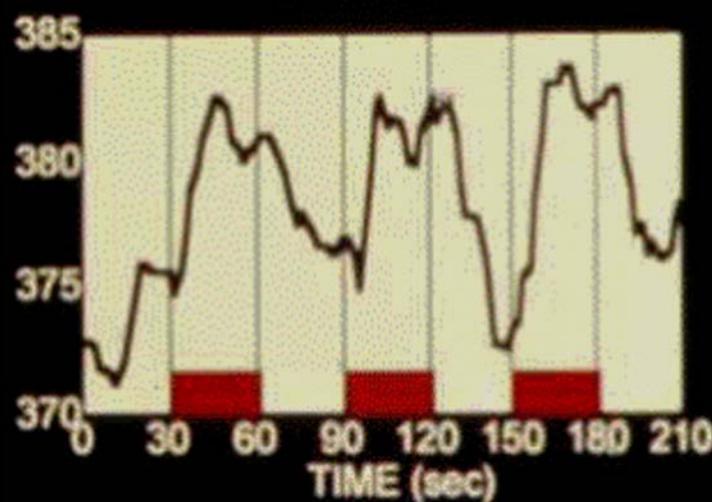
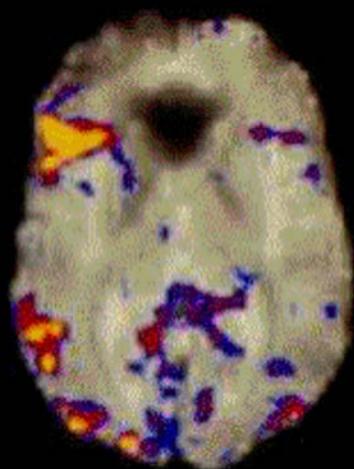
6. Free behavior Design.



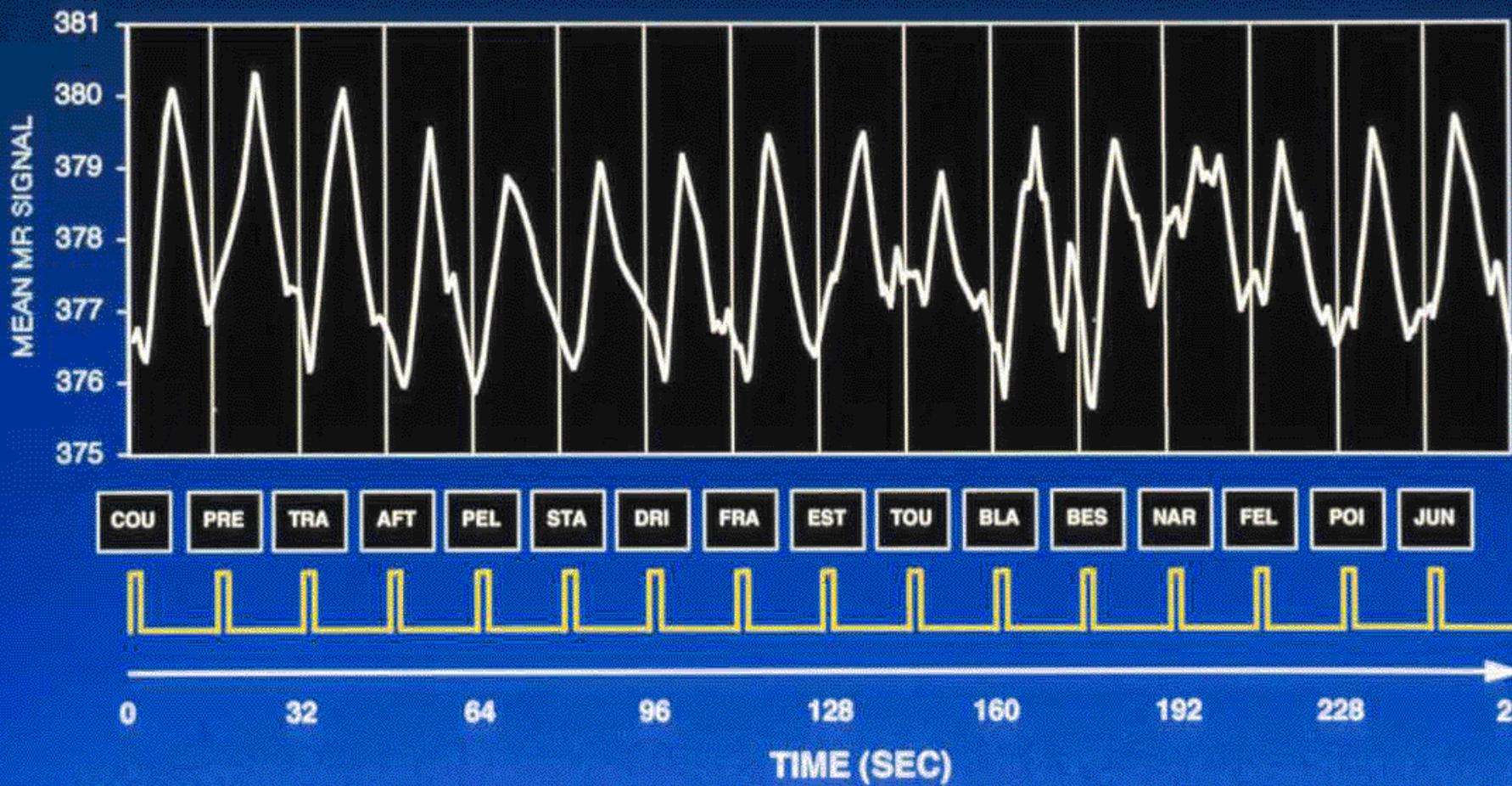
BLOCKED:



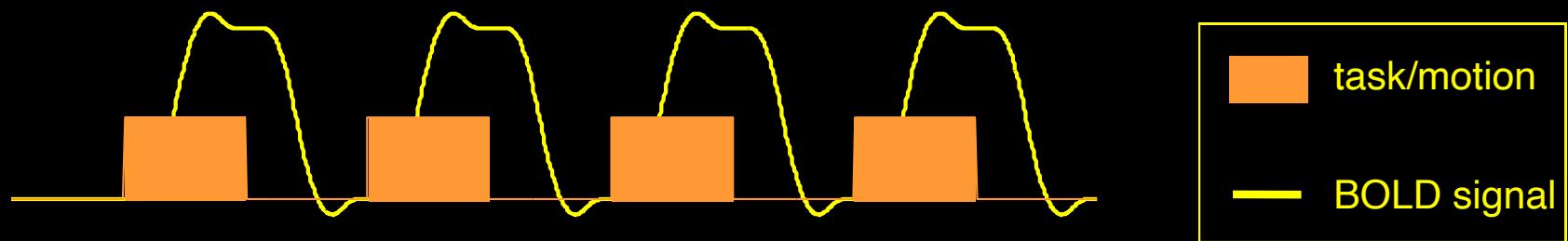
SINGLE TRIAL:



“Single-Trial” Response Across an Averaged Data Set



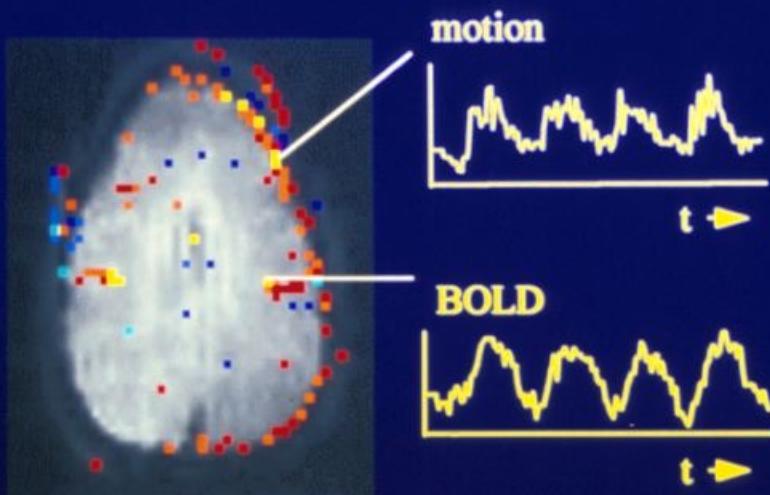
Block-trial



Single-trial (brief stimulus)

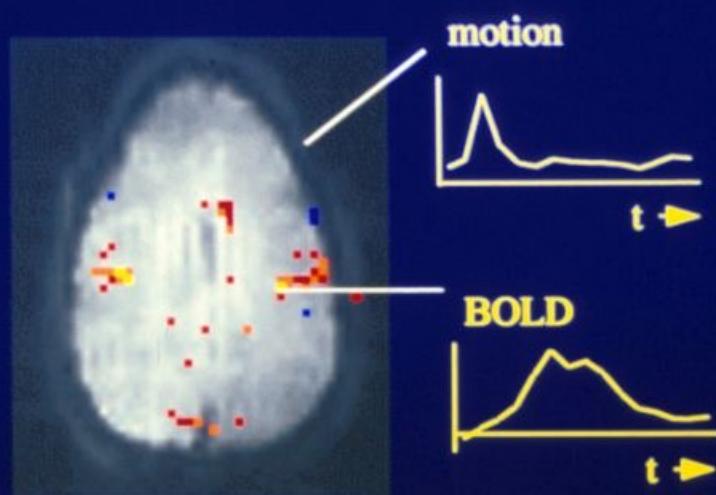


Motion-Decoupled fMRI: Functional MRI during overt word production



"block-trial" paradigm

Motion induced signal changes resemble functional (BOLD) signal changes



"single-trial" paradigm

Motion induced and BOLD signal changes are separated in time

R.M. Birn, et al.

Overt Word Production



2

3

4

5



6

7

8

9



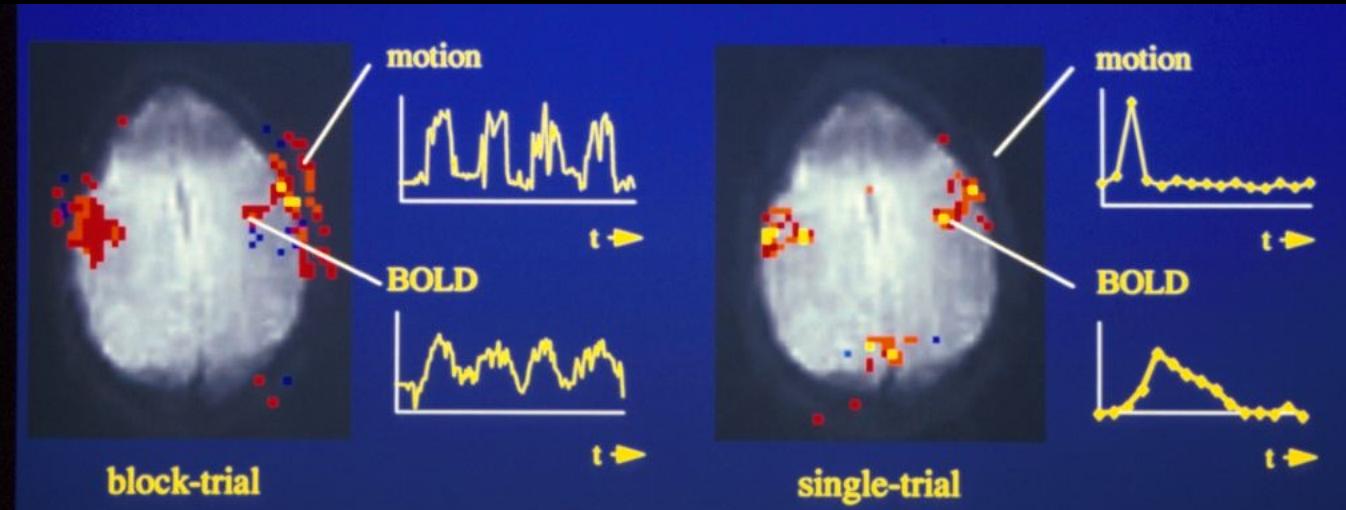
10

11

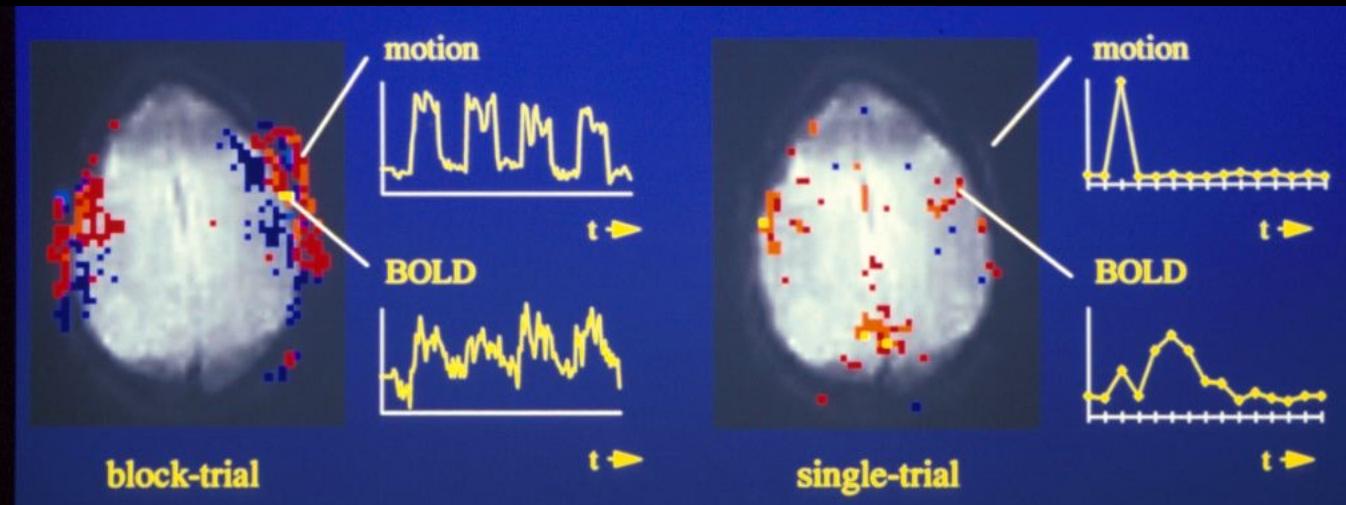
12

13

Tongue Movement



Jaw Clenching



Event-Related fMRI Questions:

- 1. What is the optimal ISI?**
- 2. How does functional contrast compare with “blocked” timing?**
(Is the hemodynamic response a linear system?)

Contrast in Event Related fMRI

Dependency on:

- Inter-stimulus Interval (ISI)**
- Stimulus Duration (SD)**

Comparison with:

- Blocked strategies**
- Synthesized responses created using convolution**

Issues:

1. ISI Issue

- Shorter ISI provides more trials per unit time.
- Shorter ISI causes overlap in hemodynamic response, reducing dynamic range.

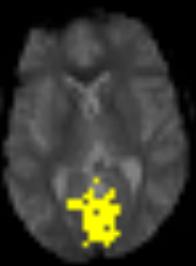
2. Contrast Issue

- Does signal behave like a linear system with brief SD?

Experimental Methods

- Two imaging planes containing motor and visual cortex.
- EPI, $3.75 \times 3.75 \times 7$ mm, TE = 40 ms, TR = 1 sec.
- Time series duration = 360 images (6 minutes).
- 10 series compared:
Single Trial: SD = 2, ISI = 24, 20, 16, 12, 10, 8, 6, 4, 2.
Blocked: SD = 20, ISI = 20.
- Subjects instructed to tap fingers when GRASS goggles were on.

Visual Cortex



ISI, SD

ISI, SD

20, 20

8, 2

12, 2

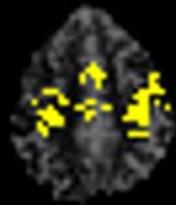
6, 2

10, 2

4, 2

2, 2

Motor Cortex



ISI, SD

ISI, SD

8, 2

20, 20

6, 2

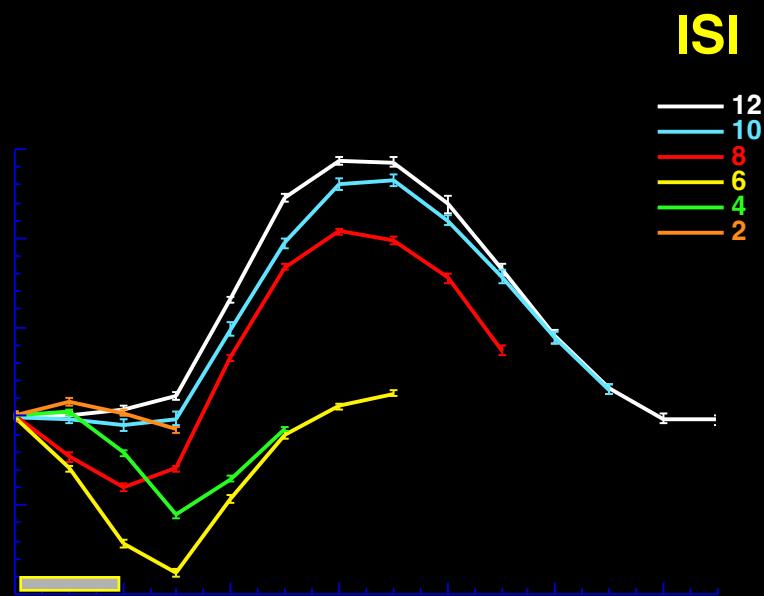
12, 2

4, 2

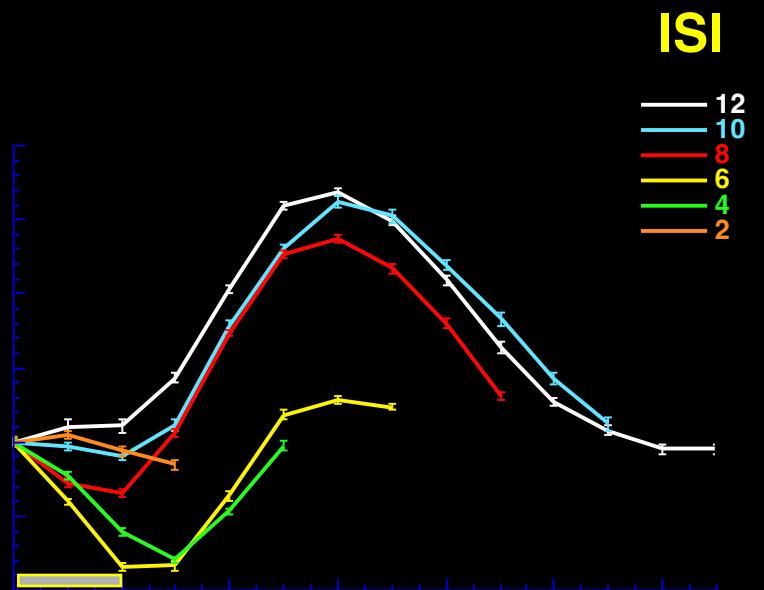
10, 2

2, 2

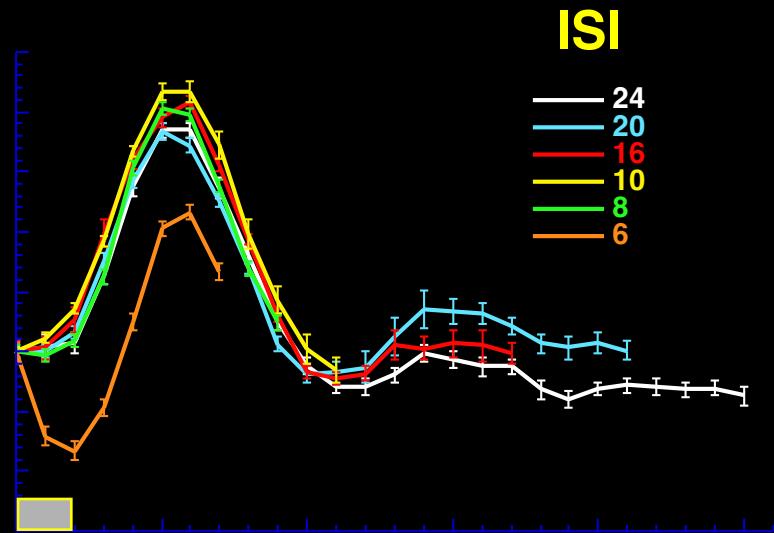
Motor Cortex



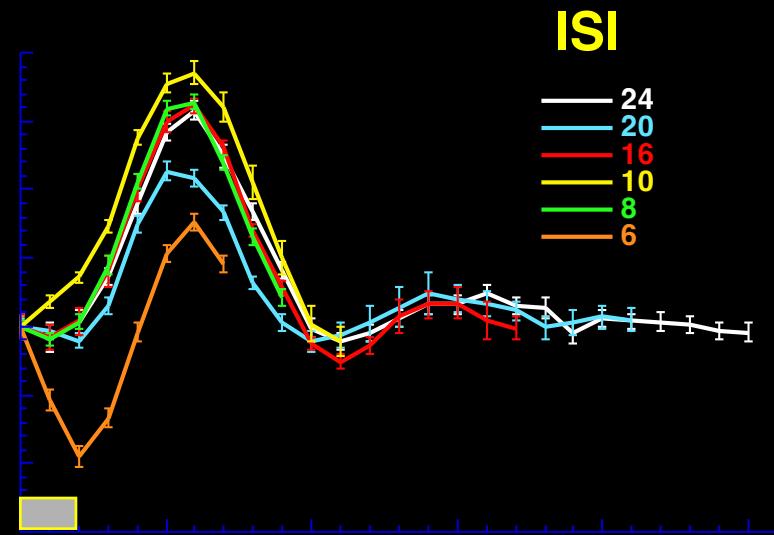
Visual Cortex



Motor Cortex



Visual Cortex

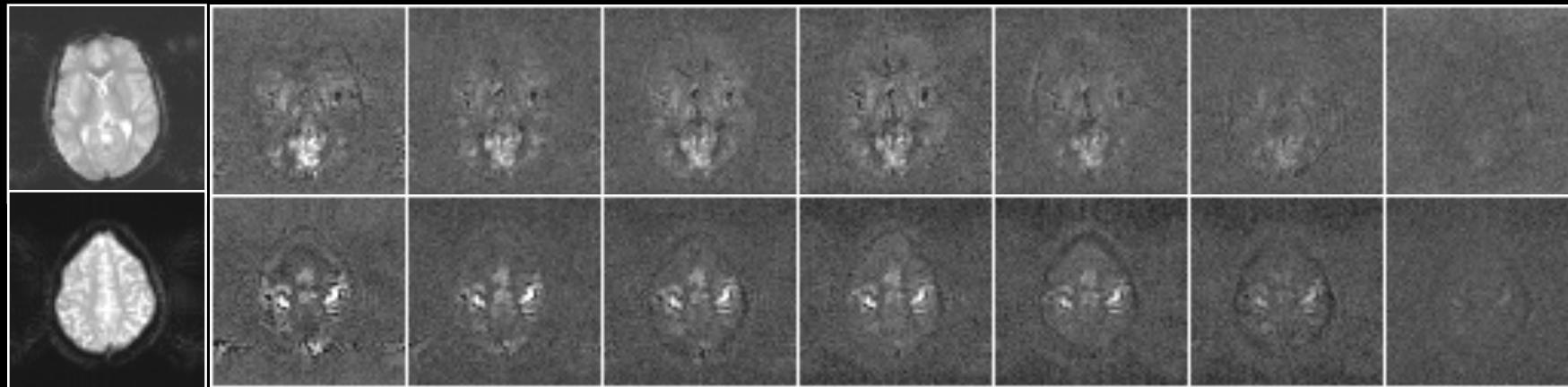


Contrast to Noise Images

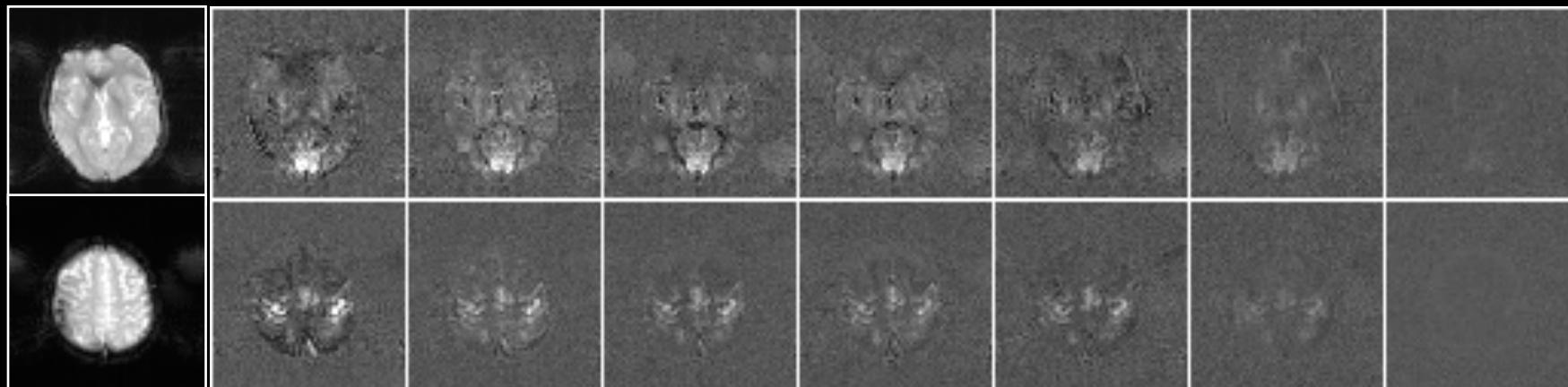
(ISI, SD)

20, 20 12, 2 10, 2 8, 2 6, 2 4, 2 2, 2

S1



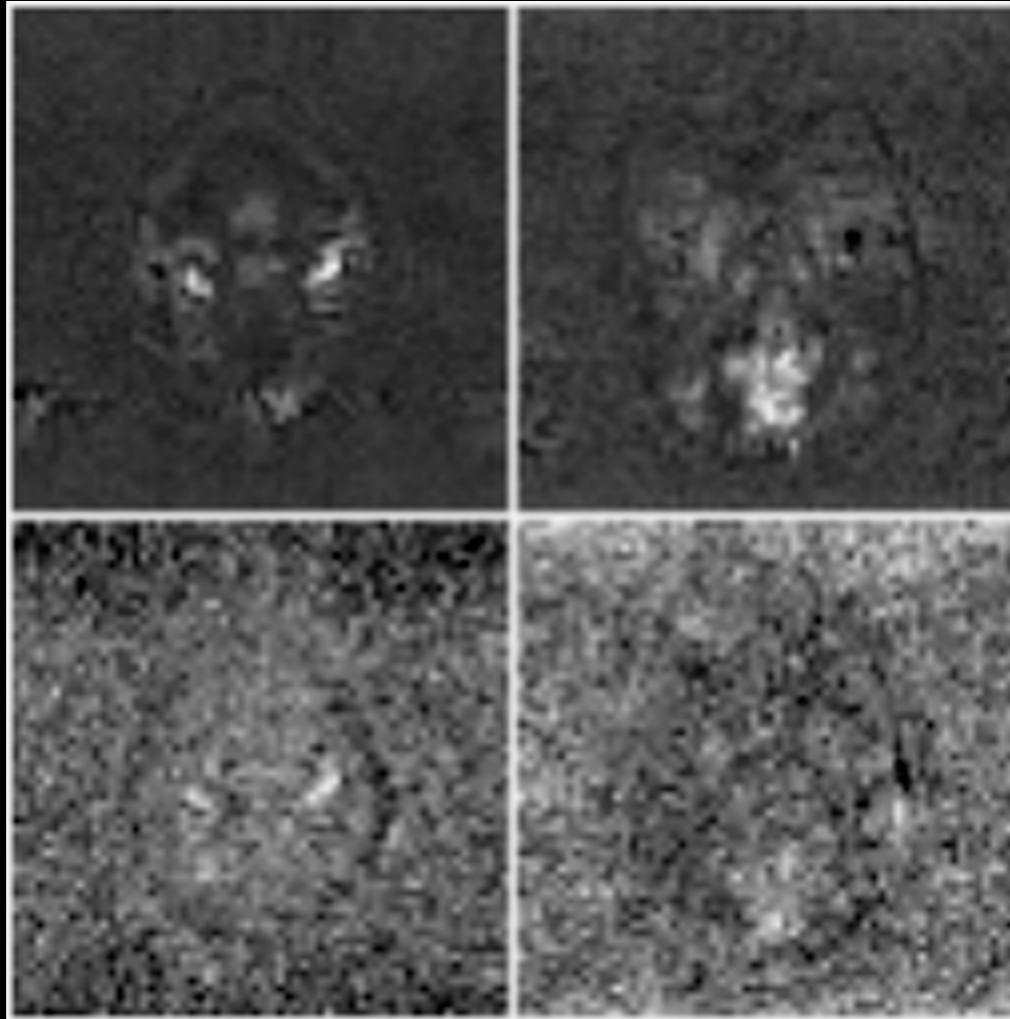
S2



Motor Visual

(ISI, SD)

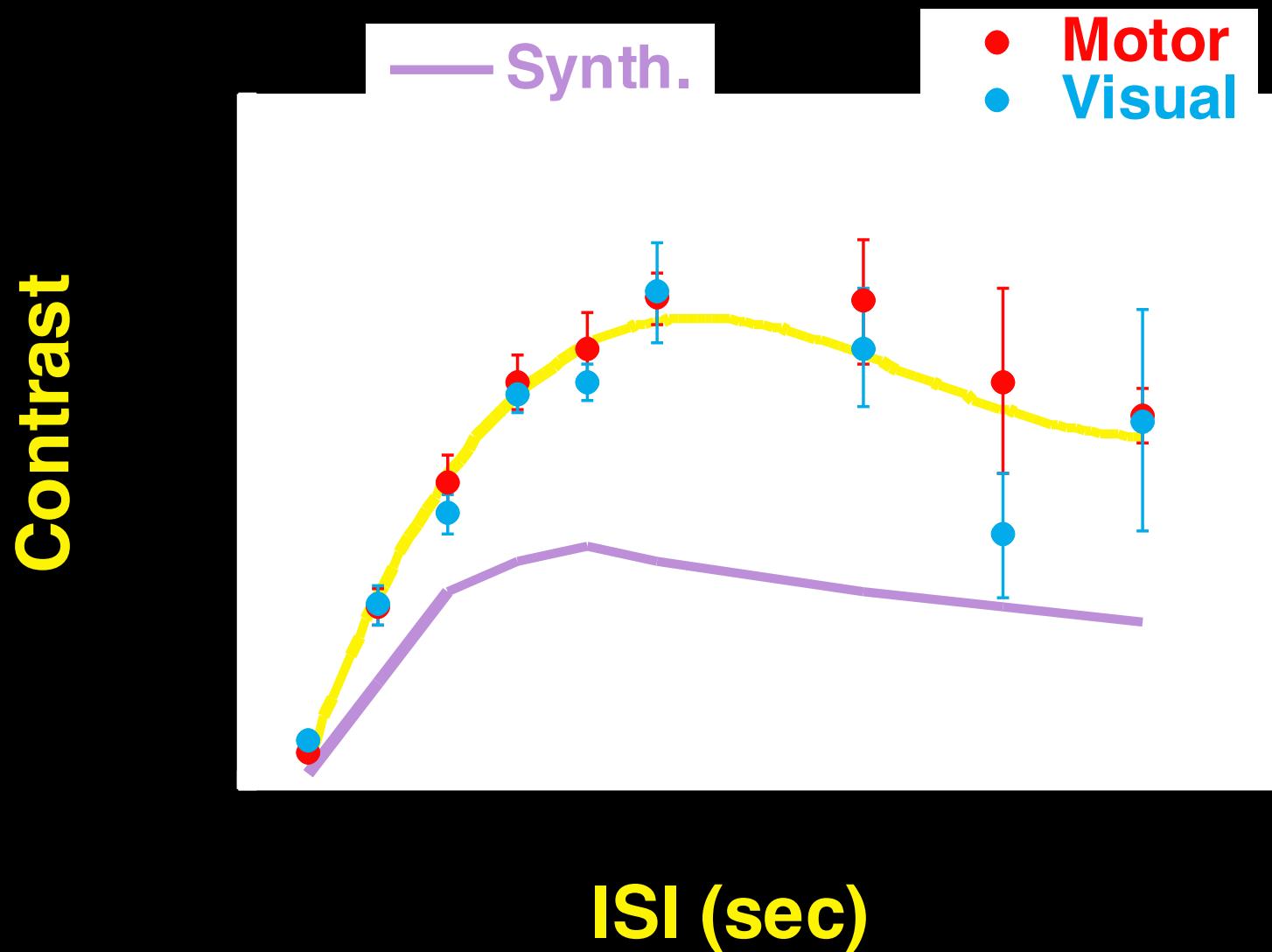
20, 20



2, 2

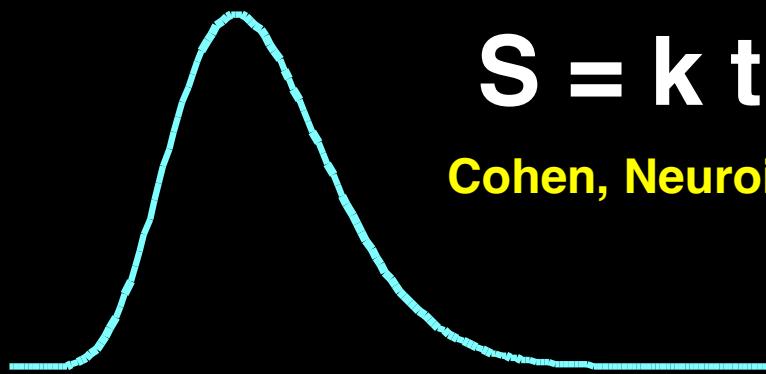
Relative differences in activation intensities may reflect spatial differences in hemodynamic responsivity. (draining veins vs. capillaries).

Functional Contrast



(Block design = 1)

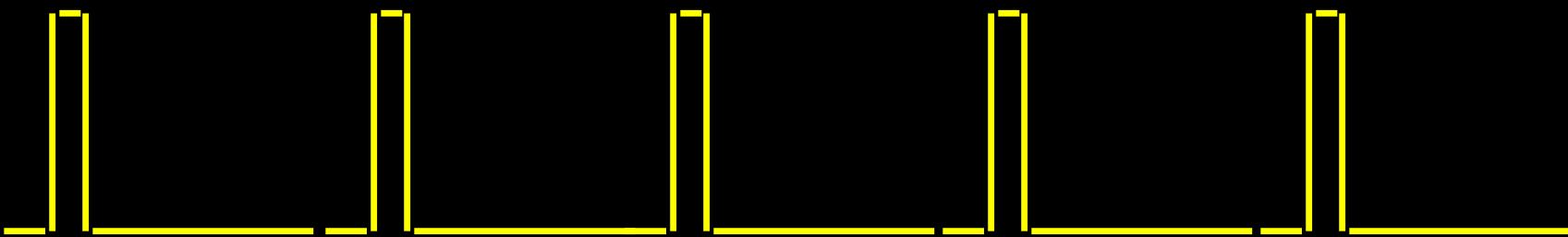
Response Synthesis



$$S = k t^{8.6} e^{-t/0.547}$$

Cohen, Neuroimage 6, 93-103 (1997)

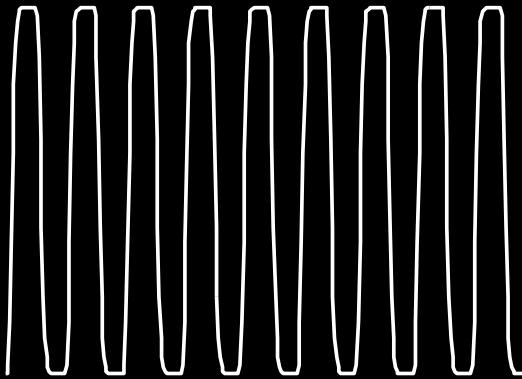
*



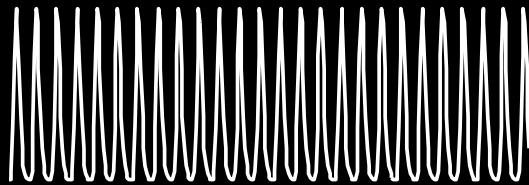
Synthesized Responses

ISI, Dur

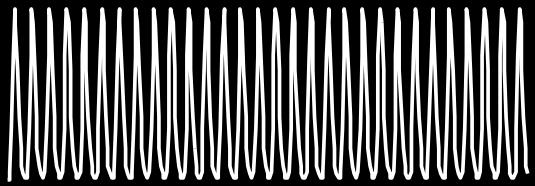
20, 20



12, 2

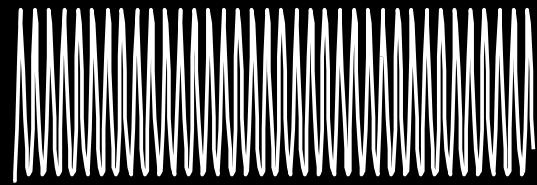


10, 2

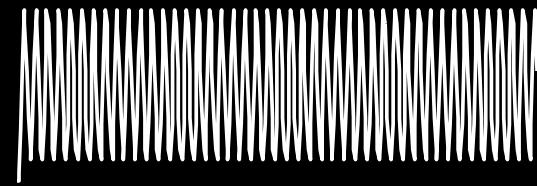


ISI, Dur

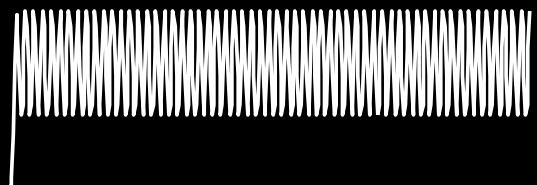
8, 2



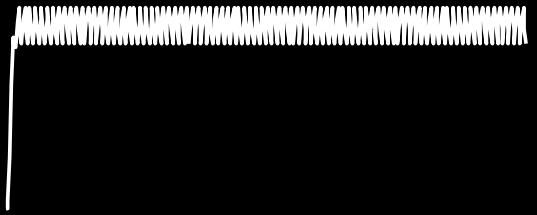
6, 2



4, 2

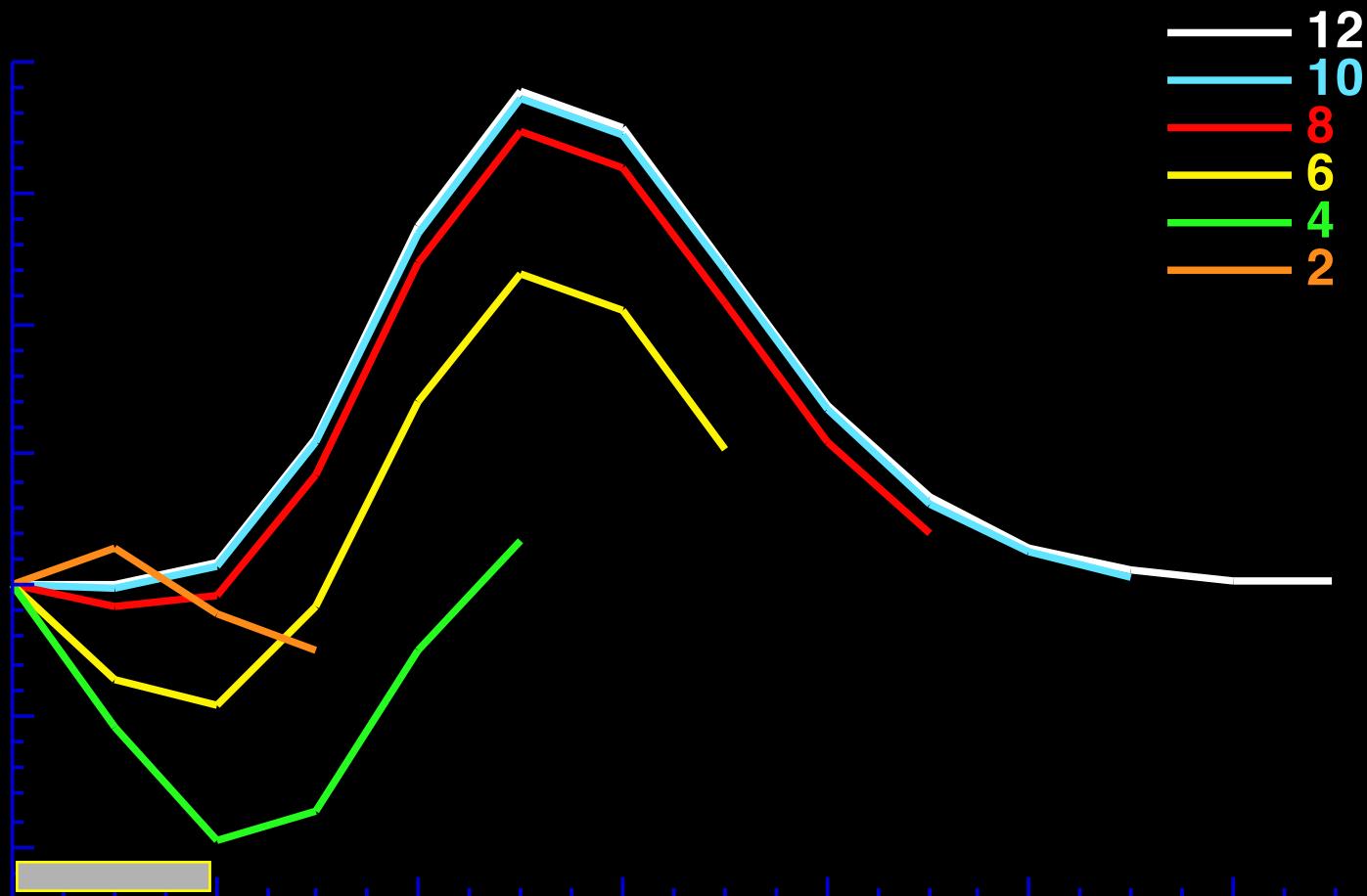


2, 2

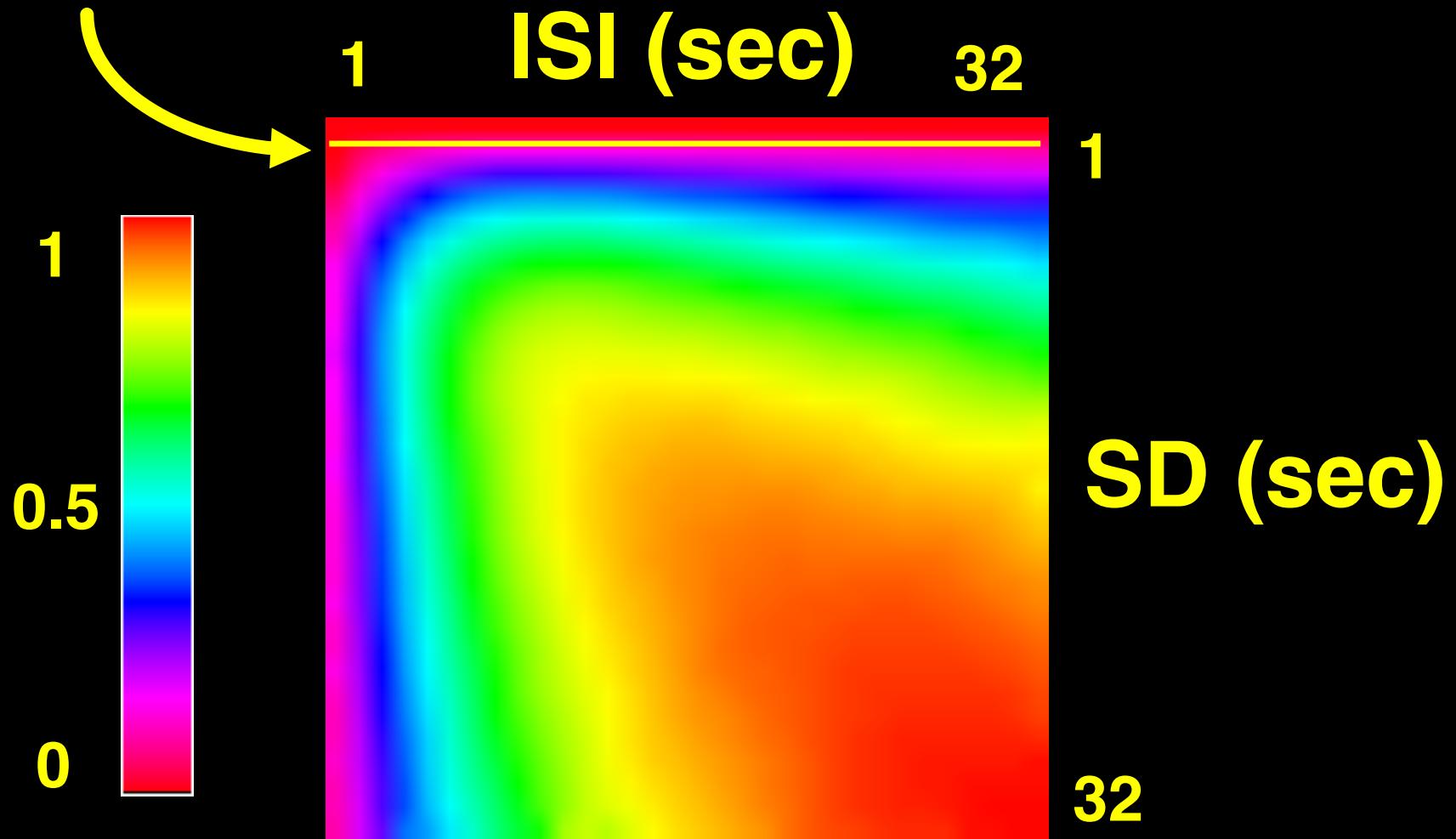


Convolution

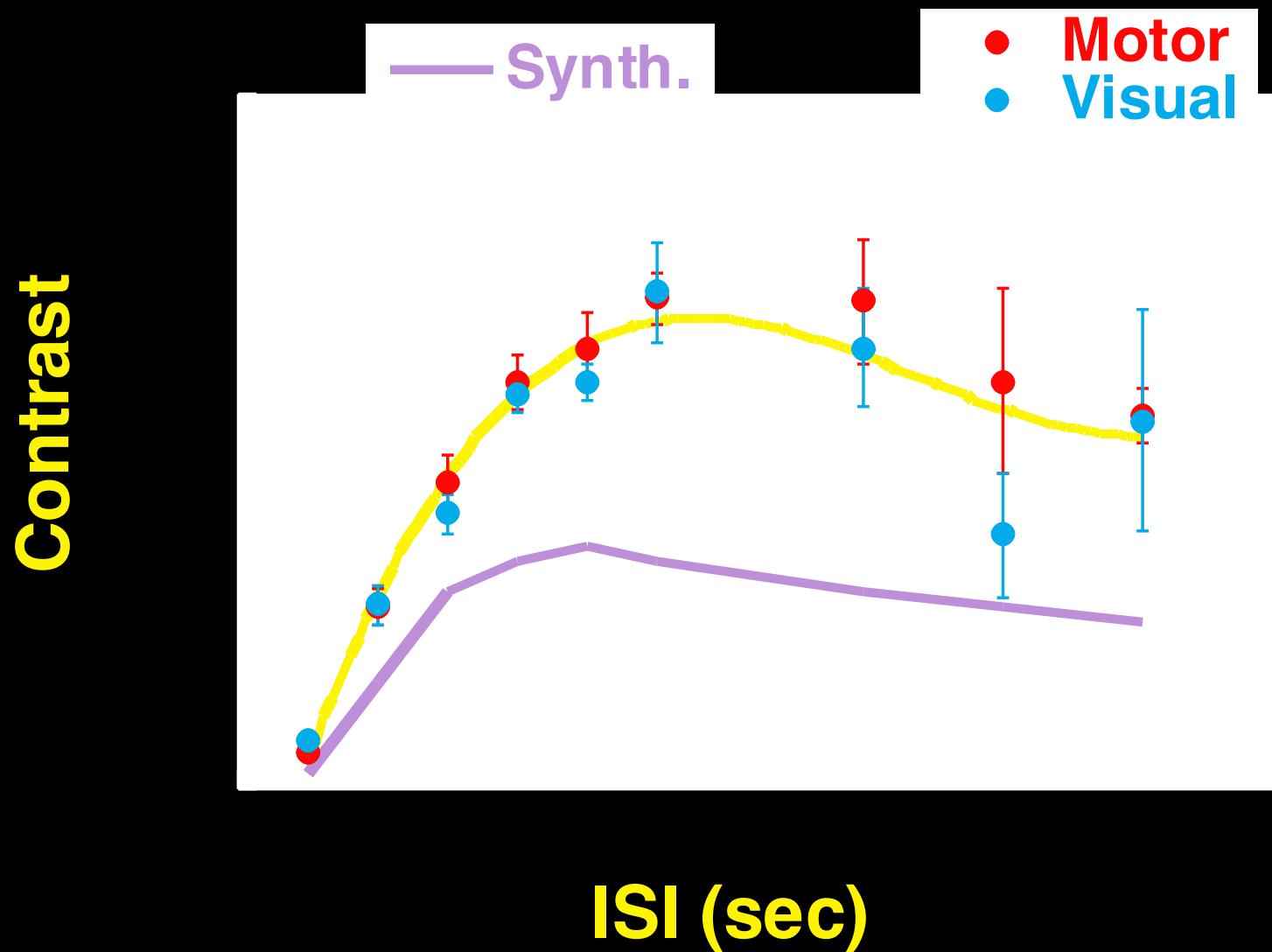
ISI



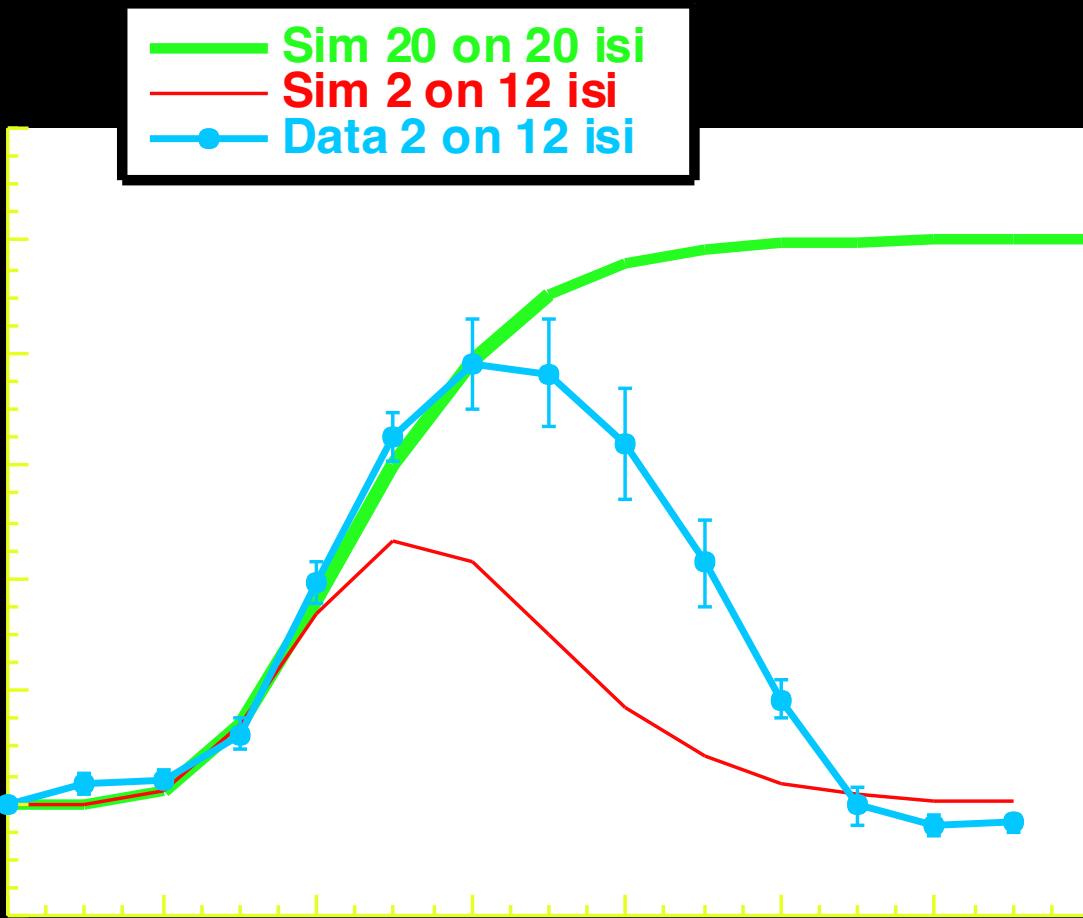
Functional Contrast



Functional Contrast



(Block design = 1)



Conclusions

- **Experimental:**

For SD = 2 sec, Optimal ISI \approx 12 sec.
Contrast = 0.65 x blocked contrast

- **Simulation using convolution:**

For SD = 2 sec, Optimlal ISI \approx 10 sec.
Contrast = 0.35 x blocked contrast

Possible reasons for greater than linear response.

Neuronal:

“Bursting” during first 100 ms.

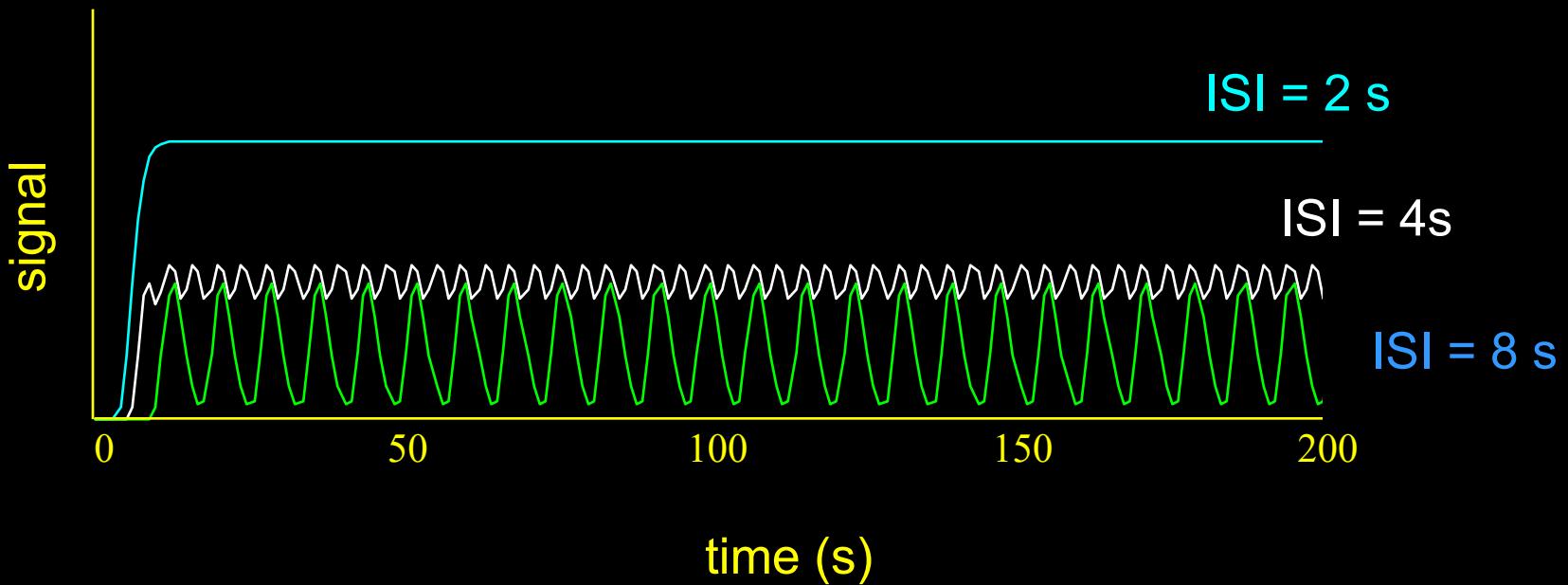
Hemodynamic/Metabolic:

Δ BV and/or Δ CMRO₂ time constants
slower than Δ Flow during initial seconds
of activation.

Possible implications for interpretation of event-related
data using short, randomized ISI w/ deconvolution.

Dale AM, Buckner RL (1997), Human Brain Mapping, 5, 329-340.

BOLD response - constant ISI



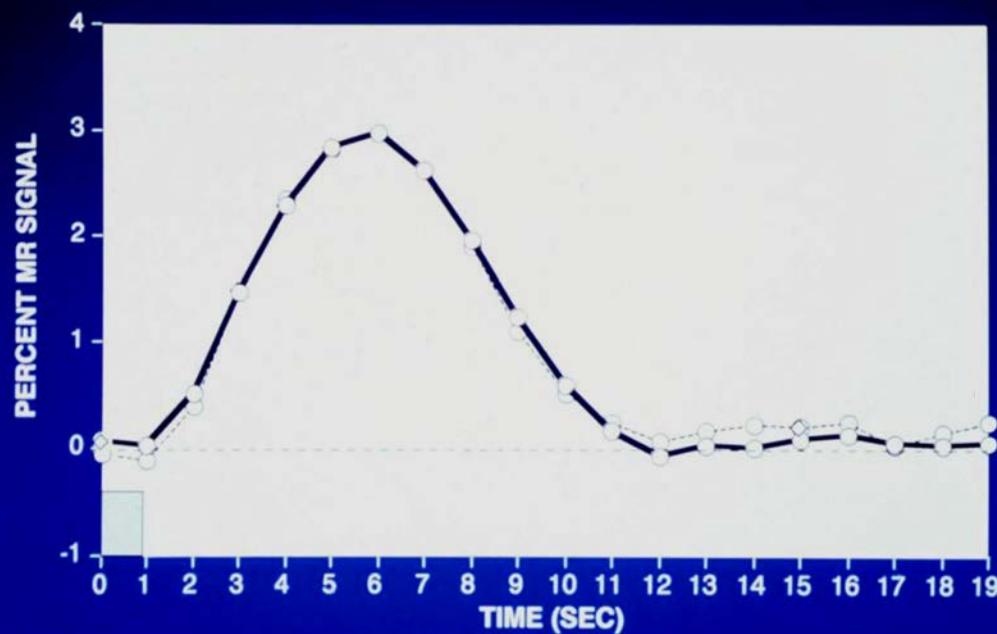
Tasks can be performed faster by varying the ISI

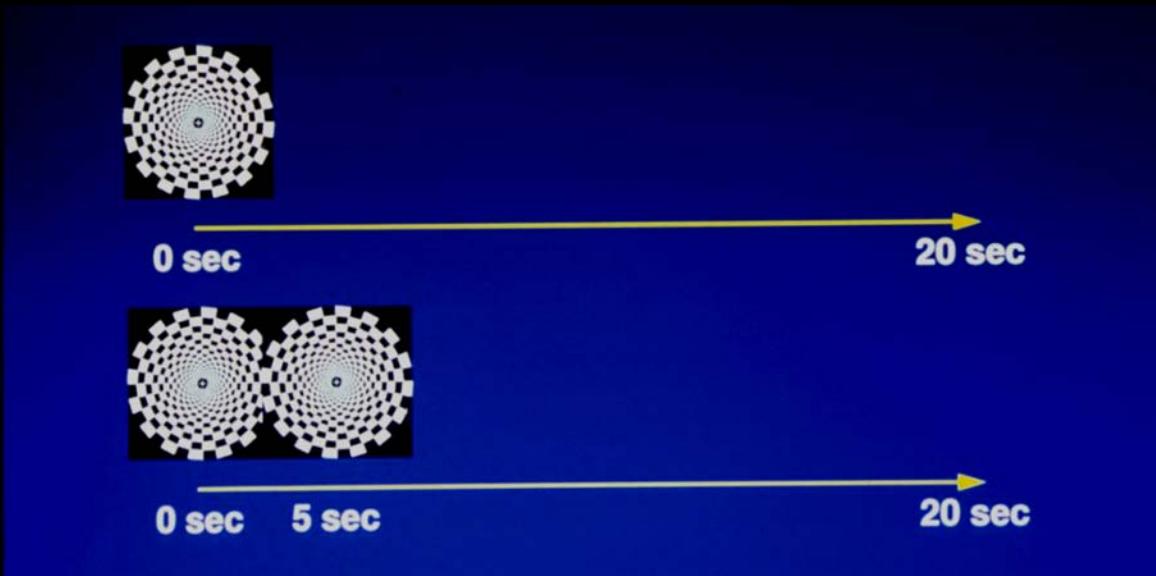


0 sec

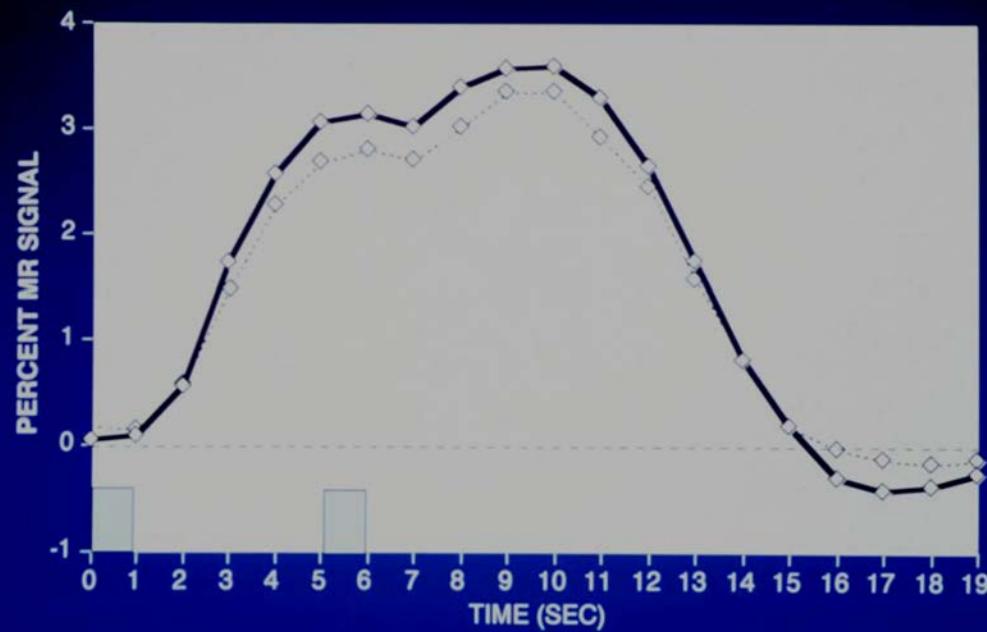
20 sec

Response to Averaged Single Trials: Subject JM

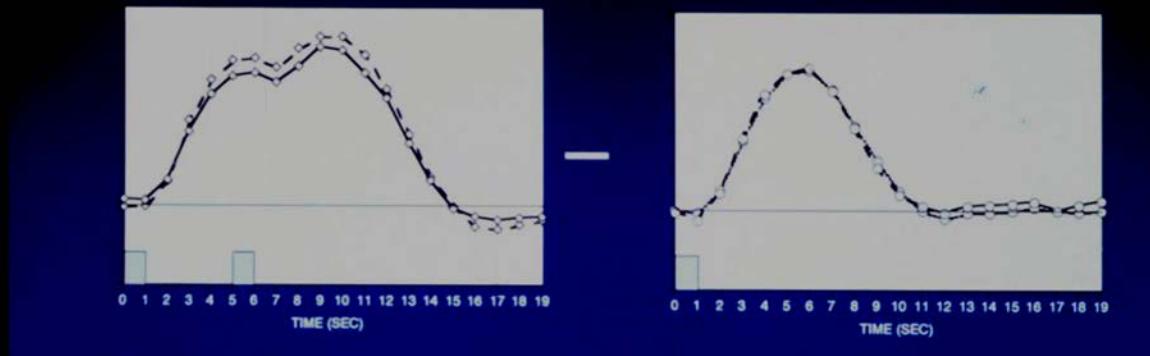




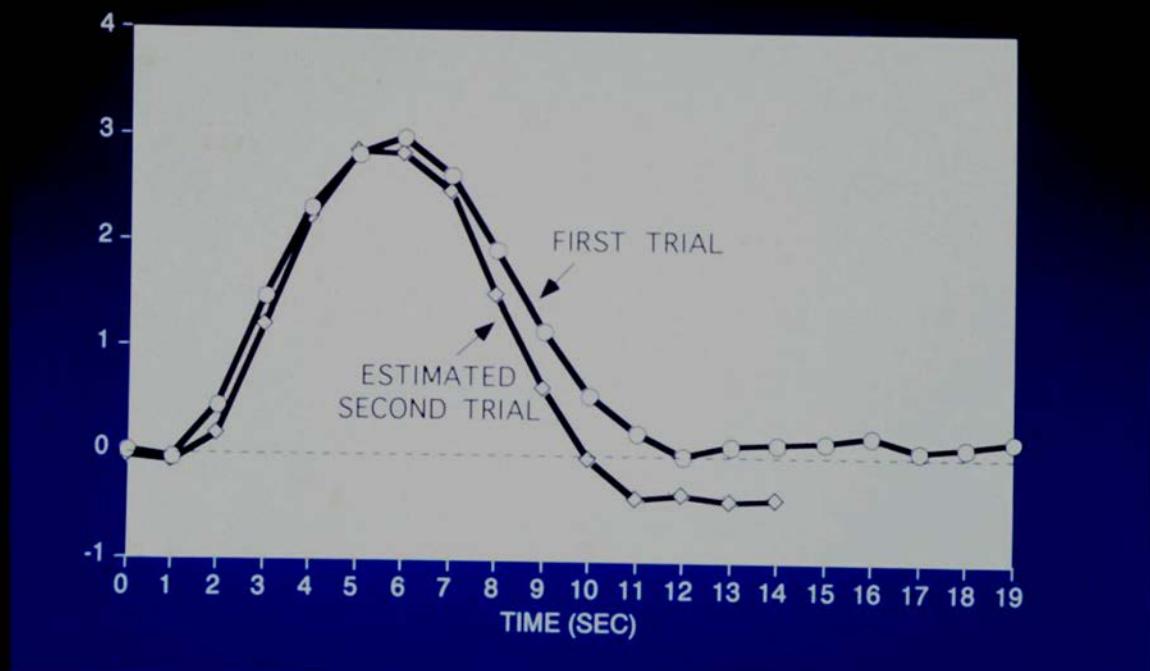
Response to Averaged Double Trials: Subject JM



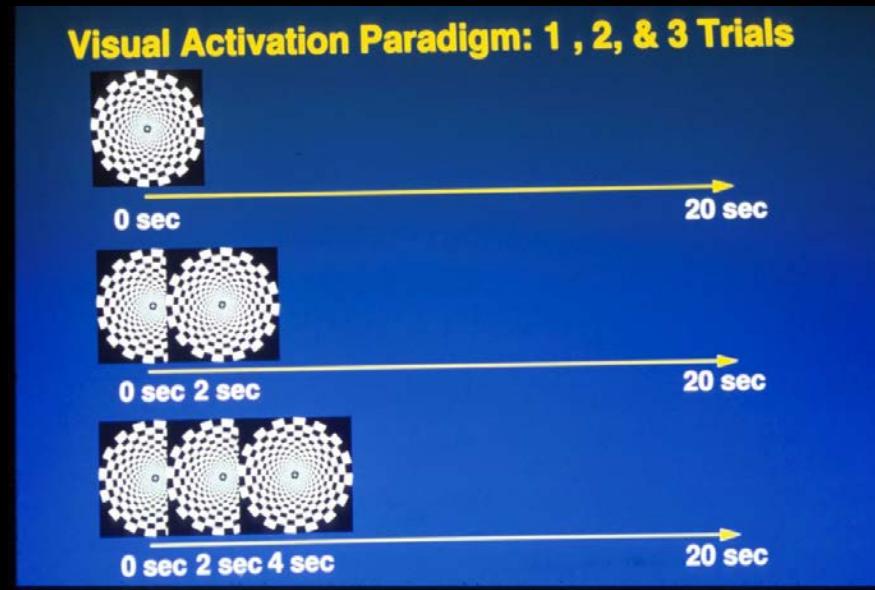
Response to Averaged Double Trials: Subject JM



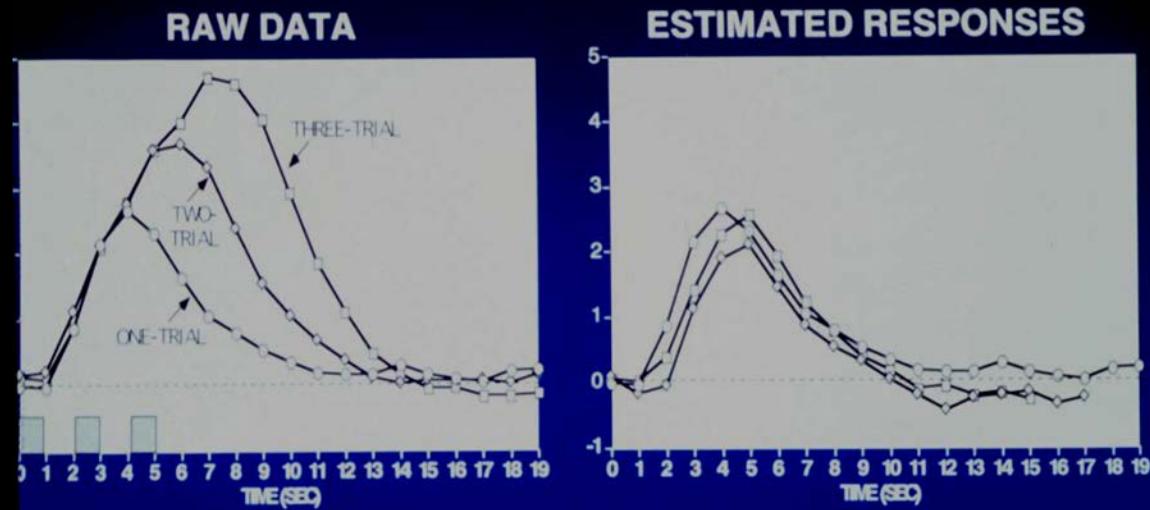
Separation of Responses: Subject JM



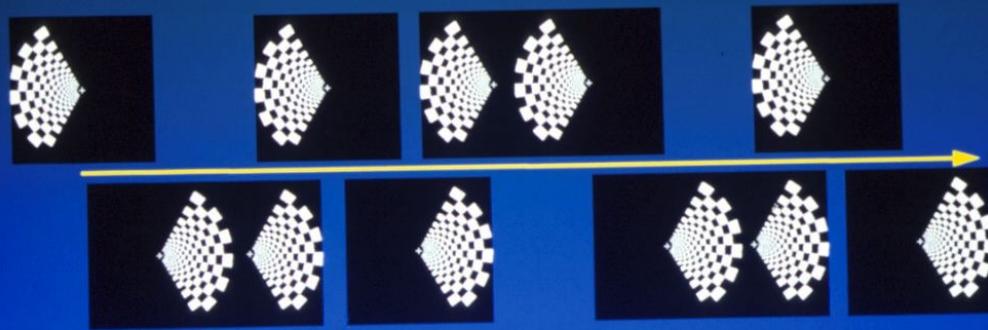
You can go
even faster with
the assumption of
linearity...



Response to Multiple Trials: Subject RW

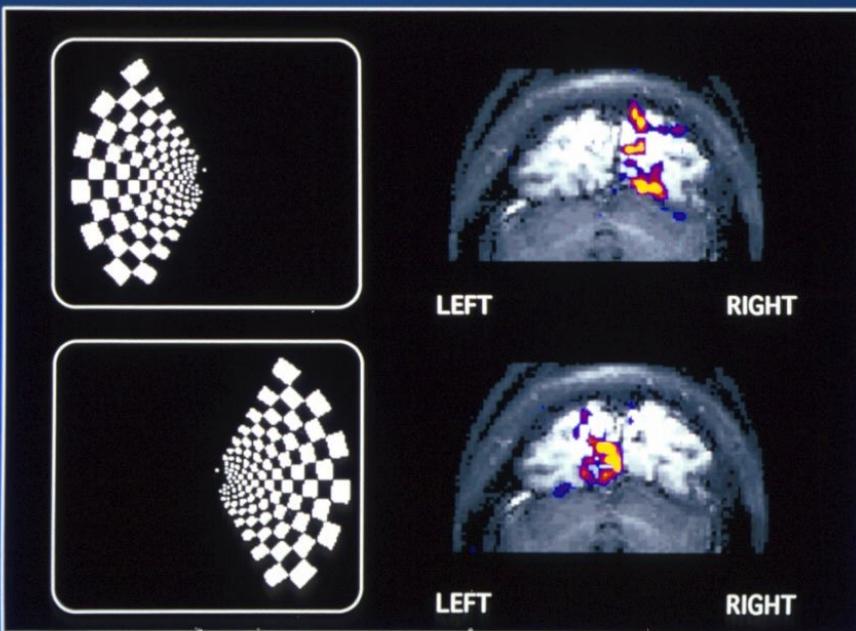


Rapid-trial Visual Activation Paradigm for Selective Averaging



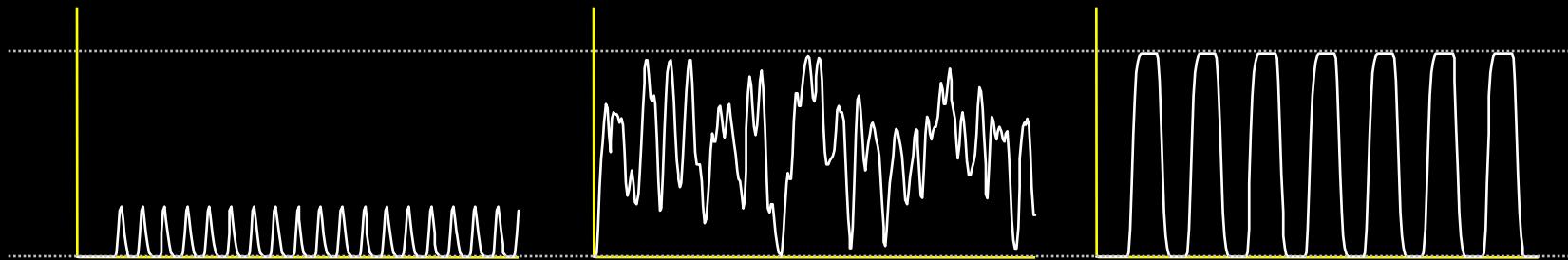
Trials randomly presented 2 sec apart

If ISI is randomized,
and if ON / OFF distribution
is 50%, the optimal average
ISI is as short as you can
make it.



BOLD response - varying ISI

BOLD response



Stimulus



Event-related
constant ISI

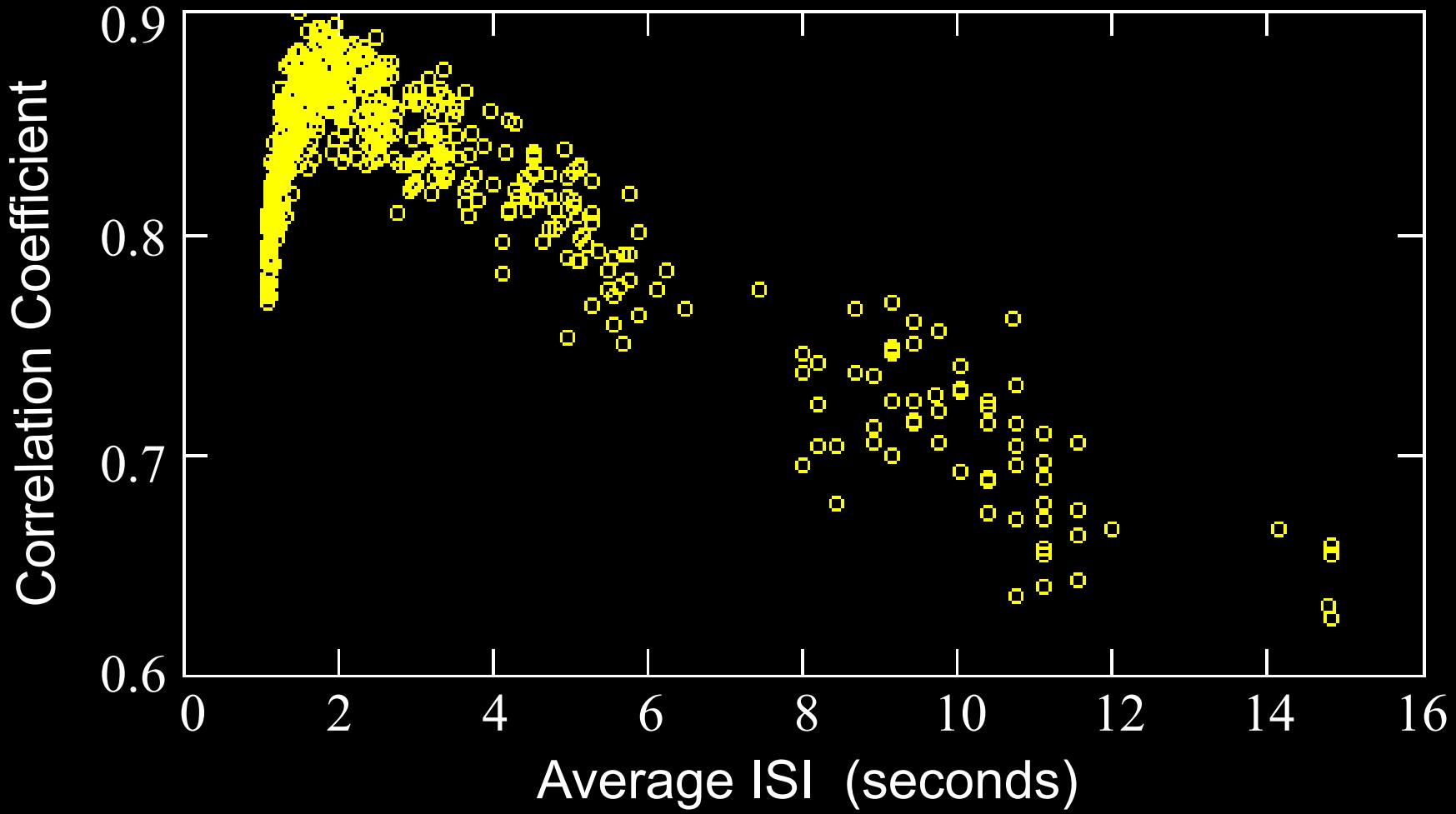


Event-related
random ISI



Blocked trial

fCNR vs. Average ISI



Conclusions

The fMRI signal is able to be calibrated. Physiologic, neuronal, and pulse sequence calibration techniques are just starting to develop to complement pulse sequence advances.

- spatial resolution** < 0.5 mm
- temporal resolution** < 100 ms
- information content:** quantitative flow, CMRO₂...

A large amount of additional information exists in the fMRI signal (i.e. fluctuations..).

To aid the development of calibration, more work needs to be done using extremely well understood neuronal activation (across several temporal, spatial, and intensity scales) to better characterize of the fMRI signal.

Neuronal Activation Input Strategies

1. Block Design

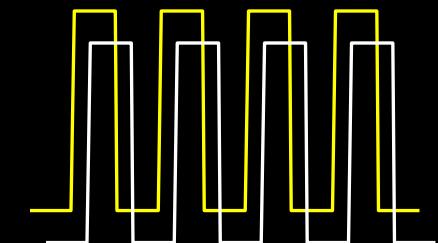
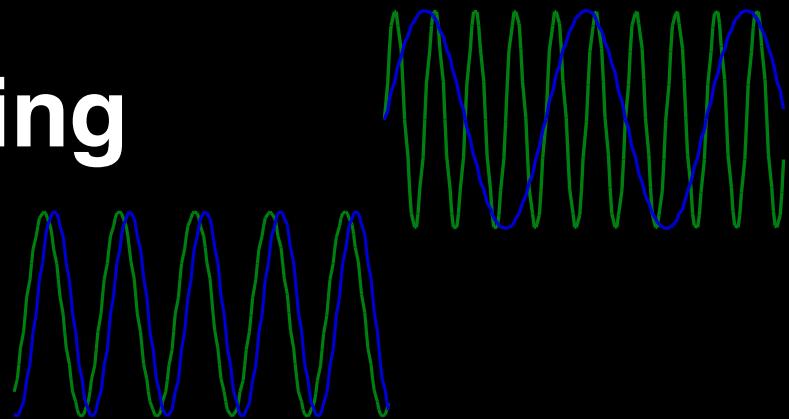
2. Frequency Encoding

3. Phase Encoding

4. Single Event

5. Orthogonal Block Design

6. Free behavior Design.



Neuronal Activation Input Strategies

1. Block Design

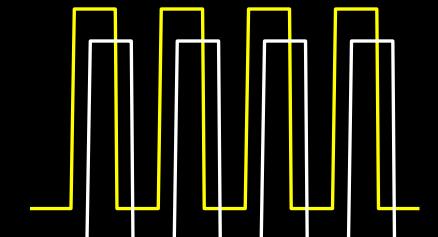
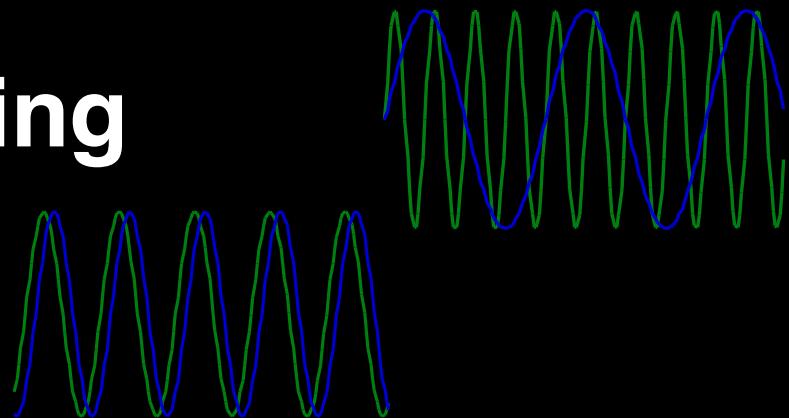
2. Frequency Encoding

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6. Free behavior Design



Free behavior Design:

Use the following as “reference functions”

- Skin Conductance
- EEG
- Eye tracking
- Task performance
- Heart rate
- Respiration rate

Pulse sequences

Basic

Shimming

RF coil arrays

Contrast comparisons

Physiologic fluctuations

Embedded contrast

Motion correction

Distortion / dropout correction

Real time fMRI

Perfusion quantitation

Effective connectivity mapping

<- Multi - modal integration ->

<- Sub - second resolution ->

<- Sub - millimeter resolution ->

<- CMRO₂ mapping ->

Processing

Parametric manipulation

Phase and freq. encoding

Orthogonal multi-task encoding

Physiologic manipulations

Event - related fMRI

Paradigms

Paradigms

Advanced

1991-1992



1992-1999



