

Choosing the Optimal Sequences and Strategies for Functional MRI

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Laboratory of Brain and Cognition
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Variables to Optimize

- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

Variables to Optimize

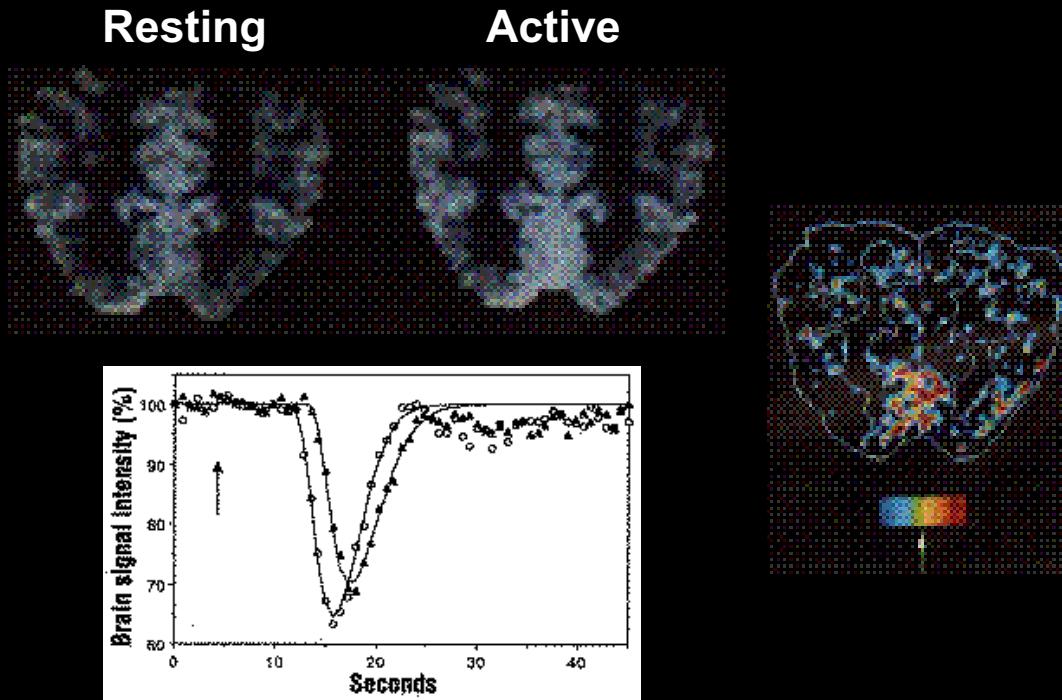
- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

Information Content

- Blood Volume
- Blood Oxygenation
- Blood Perfusion
- Hemodynamic Specificity
- Mapping of CMRO₂

Blood Volume

Contrast agent injection and time series collection of T2* or T2 - weighted images



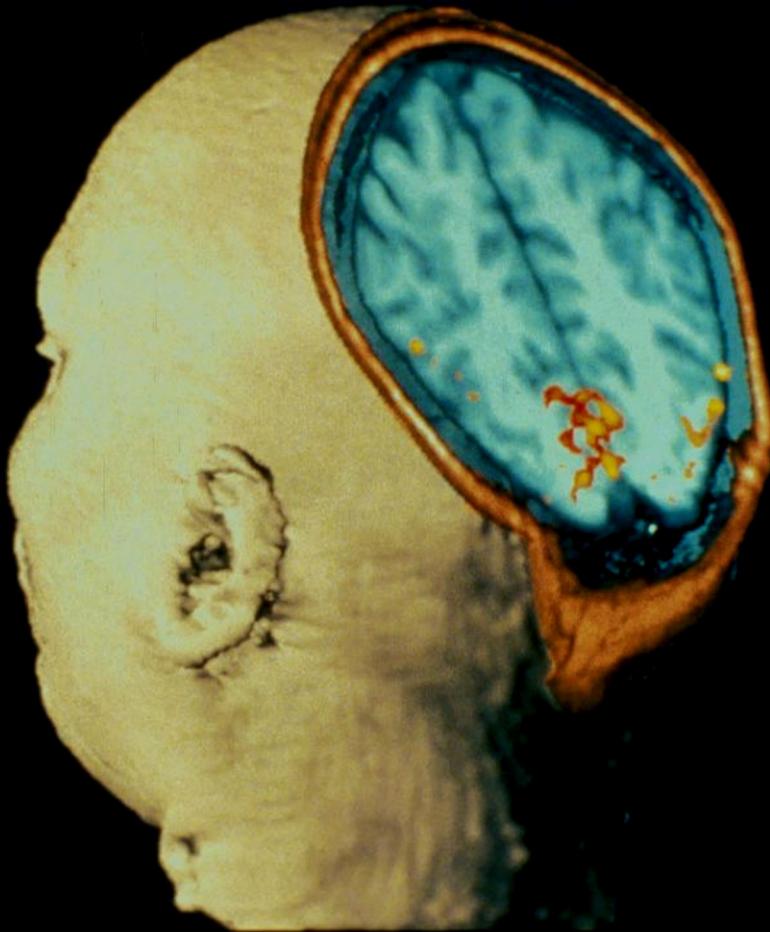
Blood Volume

**Photic
Stimulation**

**MRI Image showing
activation of the
Visual Cortex**

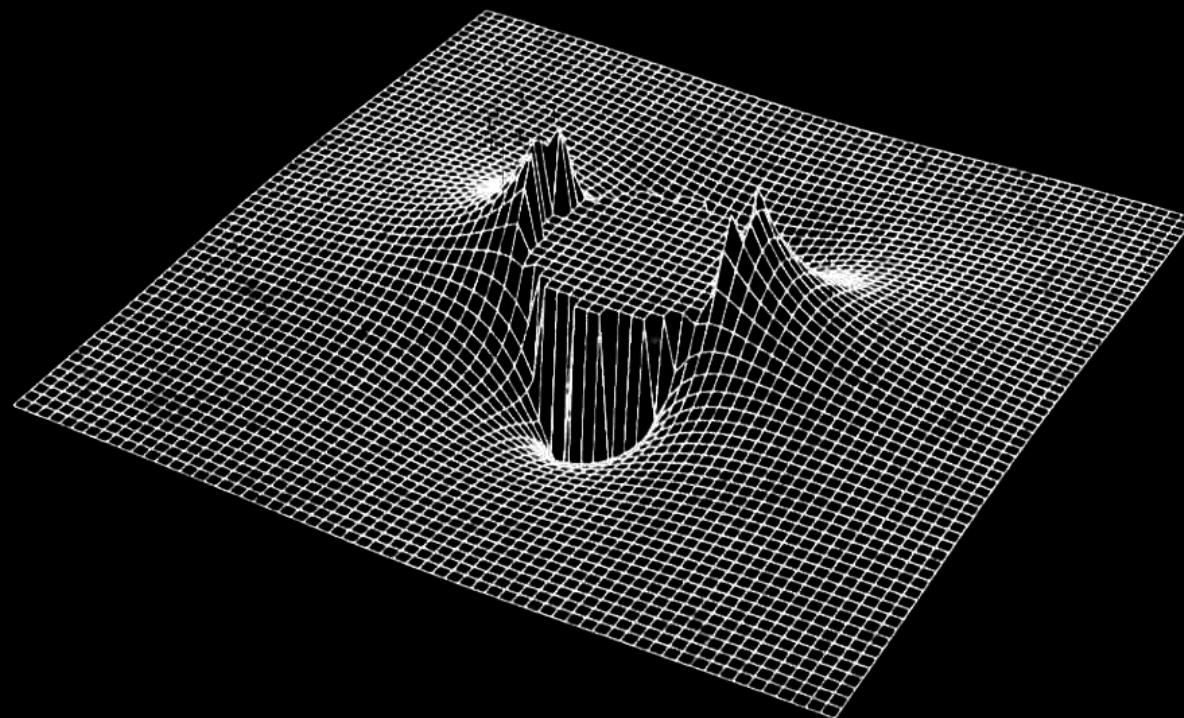
**From Belliveau, et al.
Science Nov 1991**

MSC - perfusion



Susceptibility Contrast

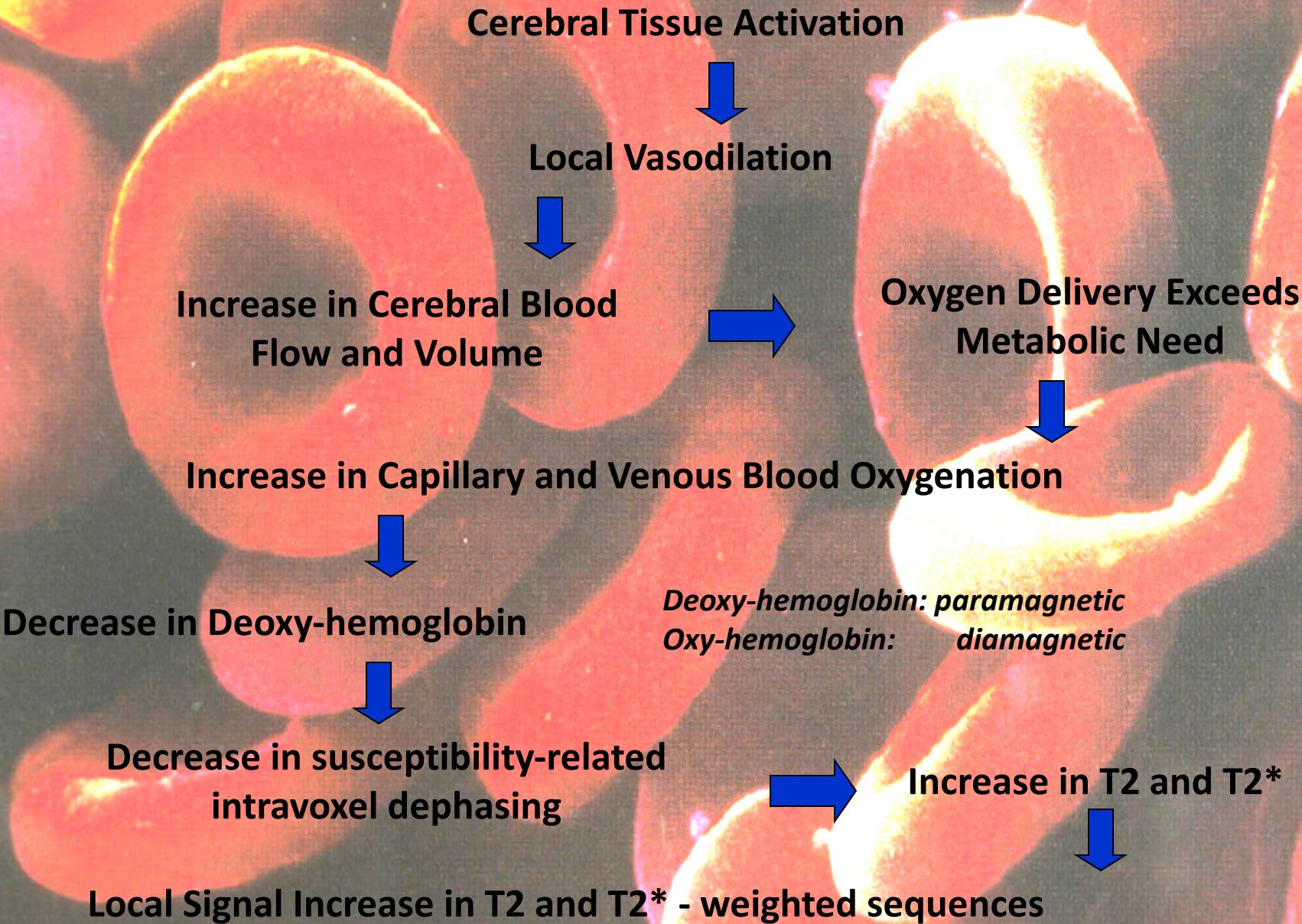
Susceptibility-Induced Field Distortion in the
Vicinity of a Microvessel \perp to B_0 .



Blood Oxygenation

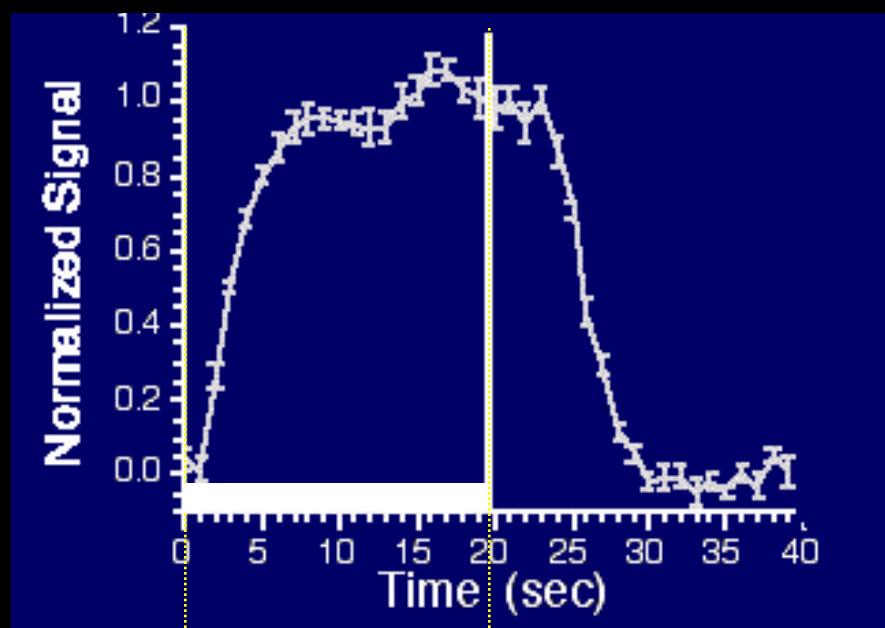


BOLD Contrast in the Detection of Neuronal Activity

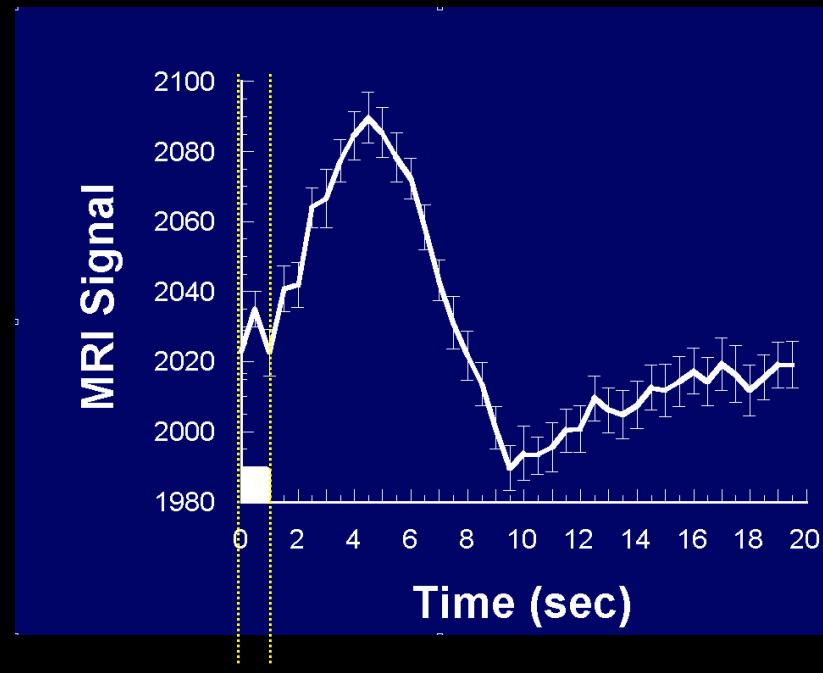


The BOLD Signal

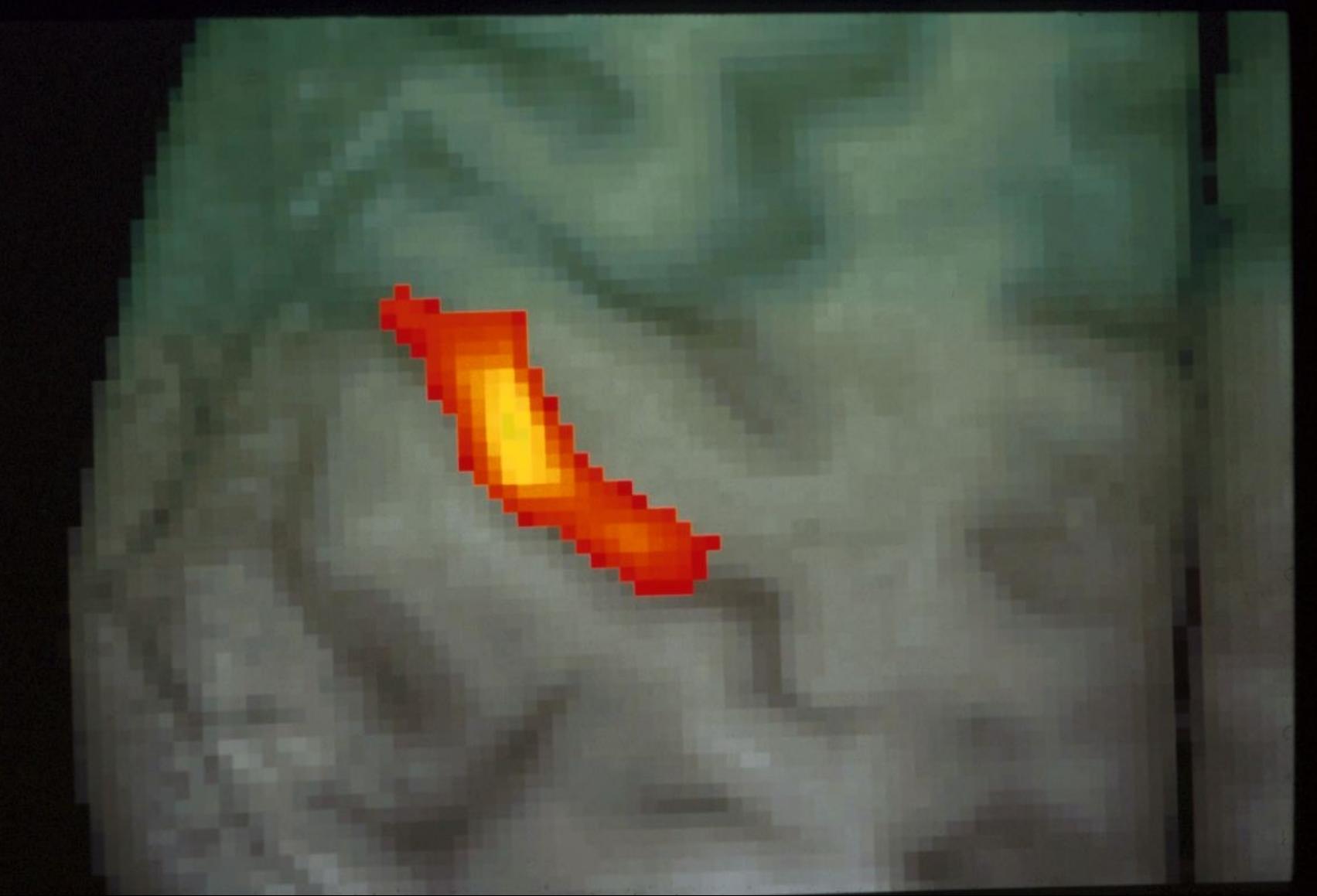
Blood Oxxygenation Level Dependent (BOLD) signal changes



task

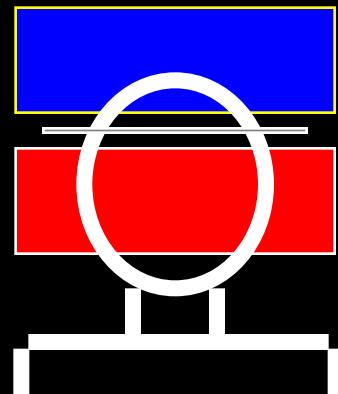


task

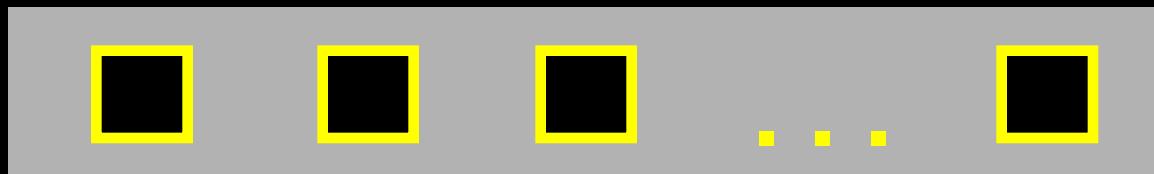
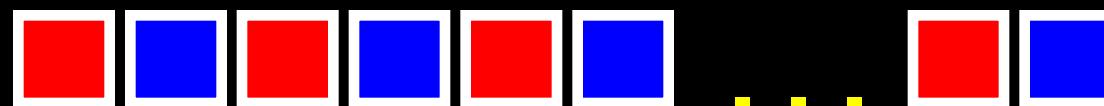
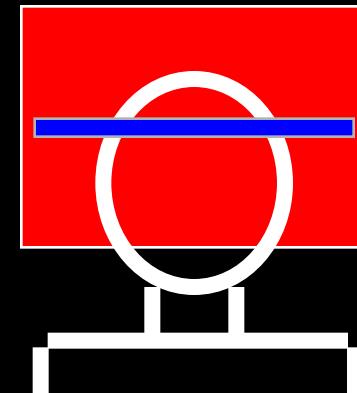


Blood Perfusion

EPISTAR



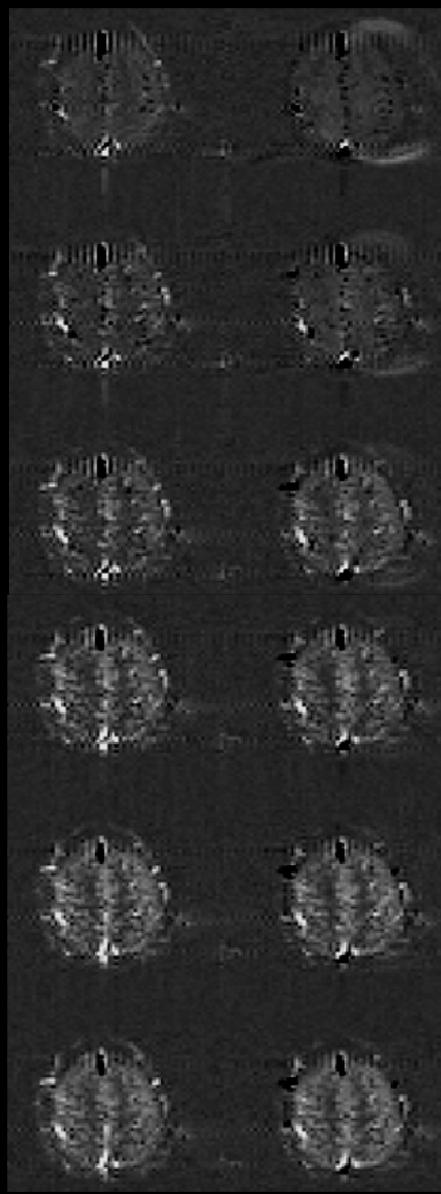
FAIR



Perfusion
Time Series

TI (ms) FAIR EPISTAR

200



400

600

800

1000

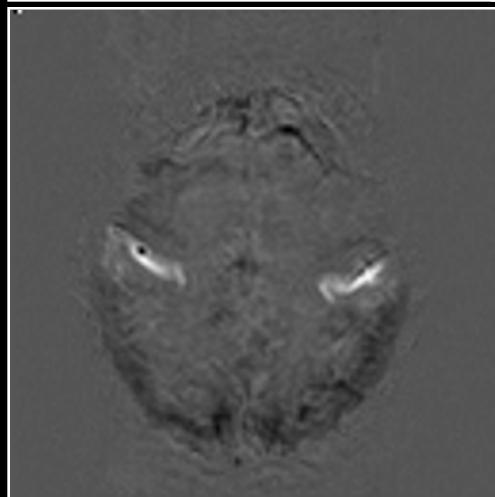
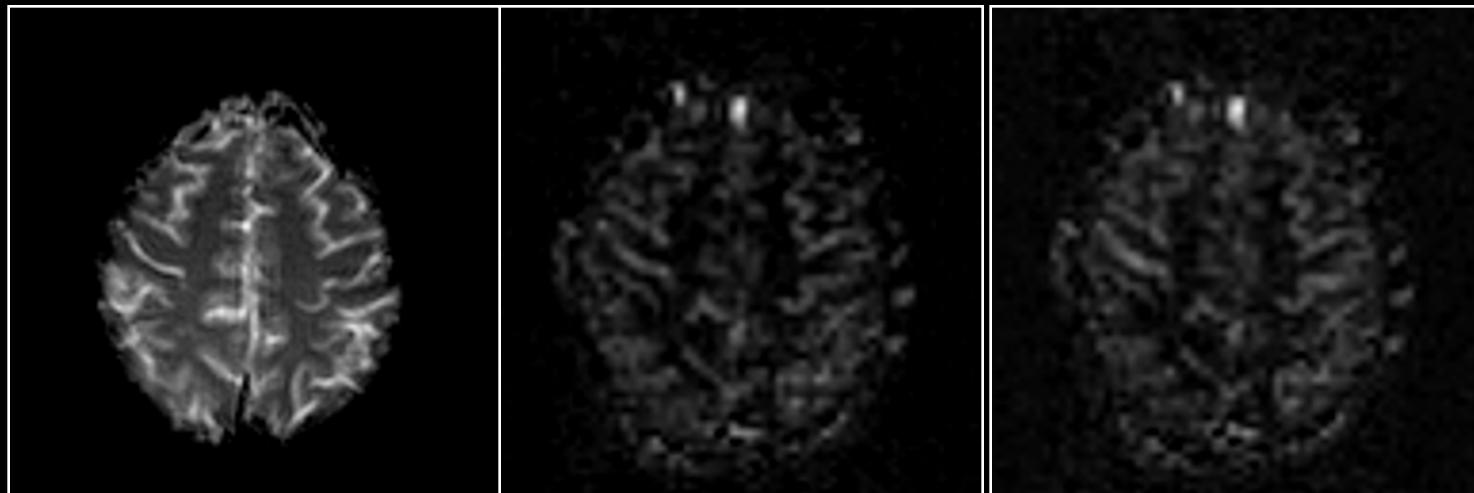
1200

Perfusion

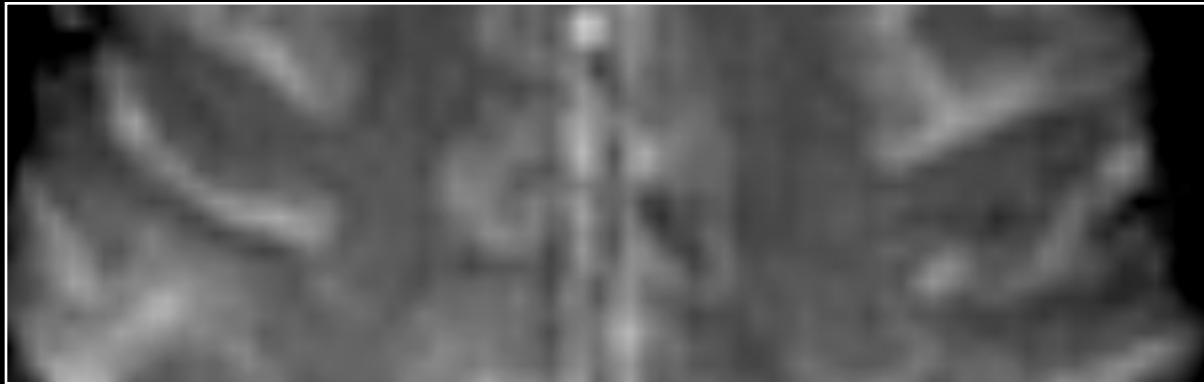
BOLD

Rest

Activation



Anatomy



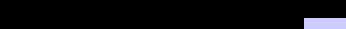
BOLD



Perfusion



Volume



- unique information
- baseline information
- multislice trivial

- invasive
- low C / N for func.

BOLD

- highest C / N
- easy to implement
- multislice trivial
- non invasive
- highest temp. res.

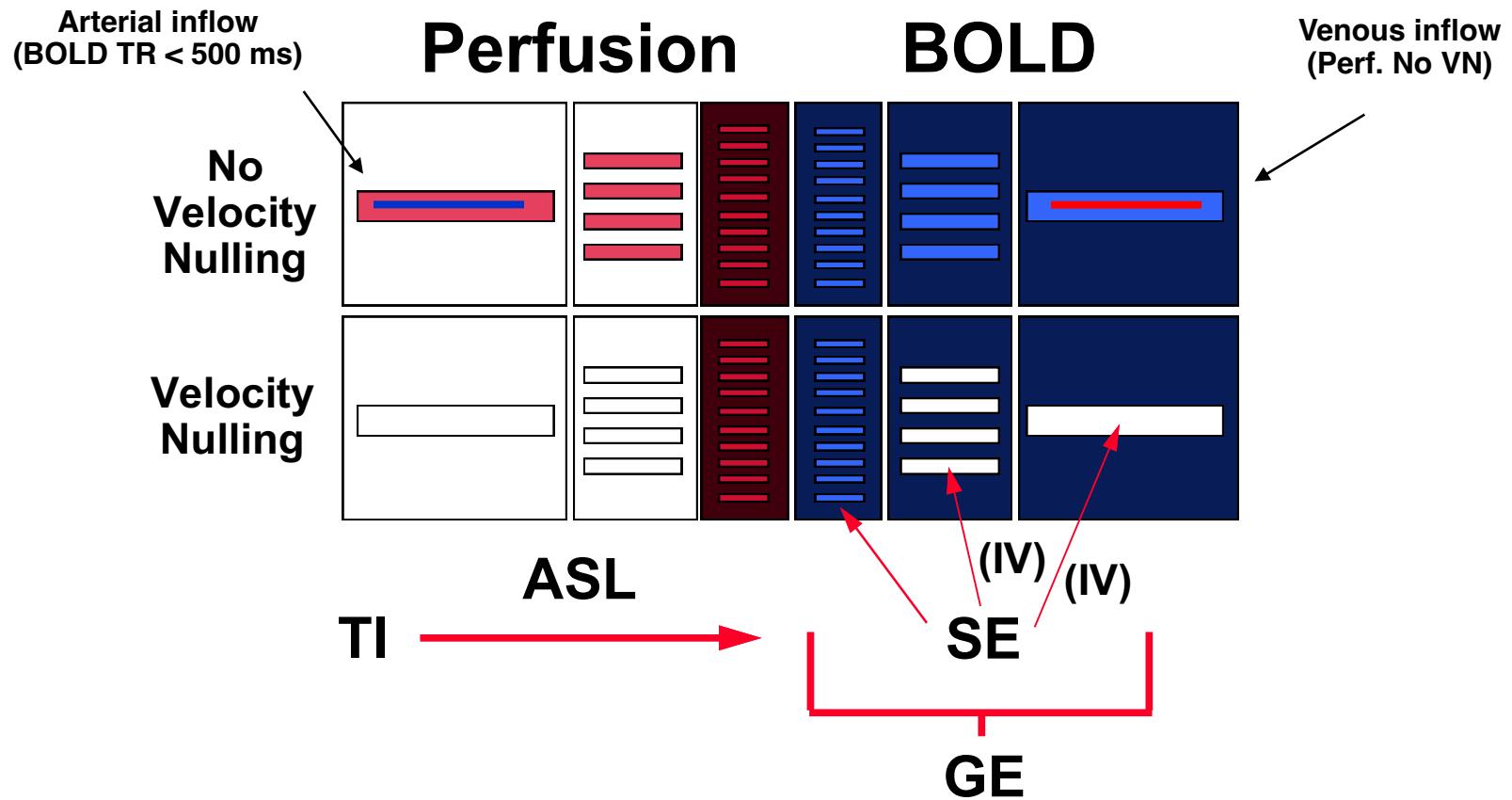
- complicated signal
- no baseline info.

Perfusion

- unique information
- control over ves. size
- baseline information
- non invasive

- multislice non trivial
- lower temp. res.
- low C / N

Hemodynamic Specificity



Mapping of CMRO₂

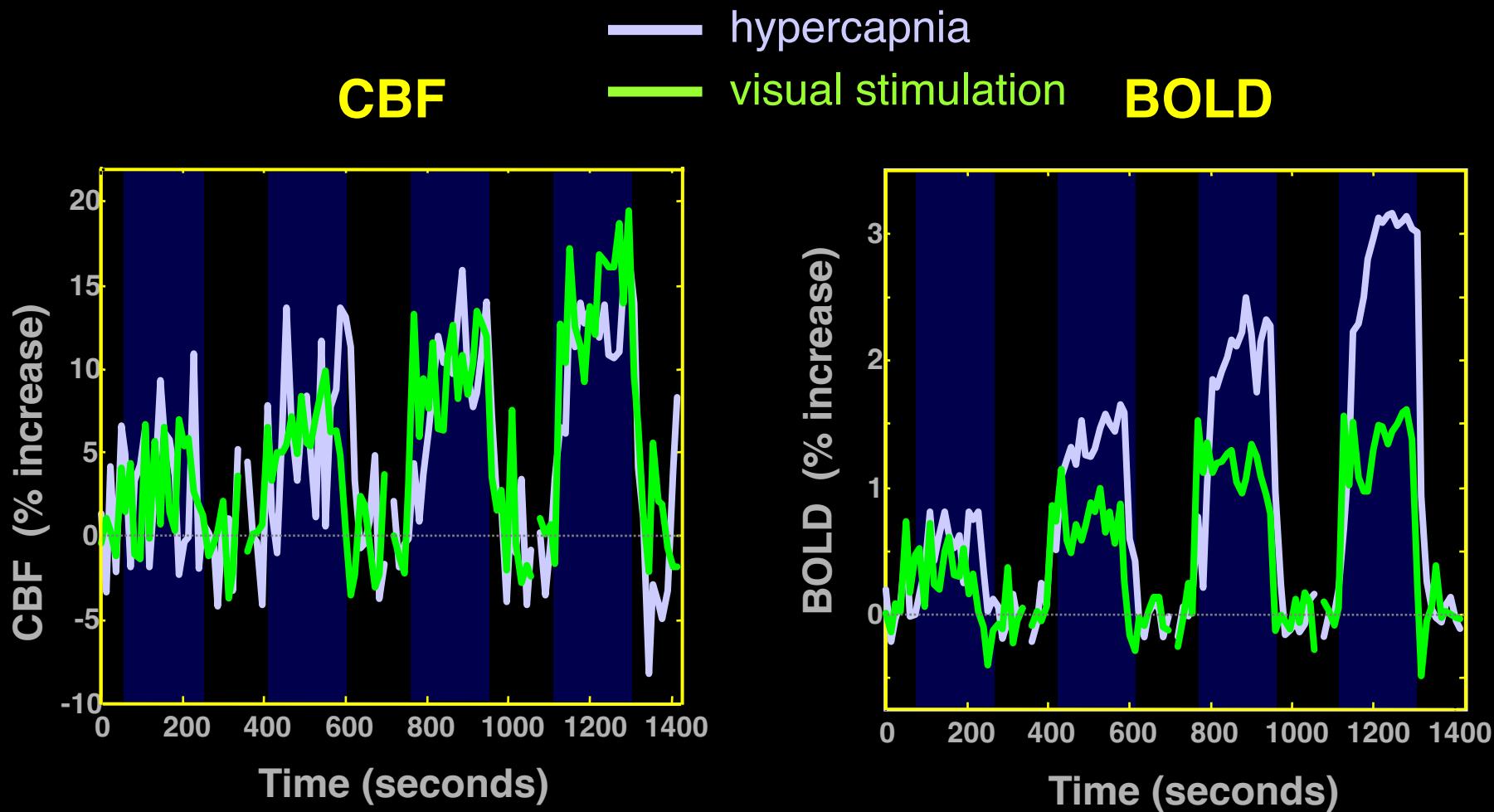
Activation:

Flow	↑↑
CMRO ₂	↑
Blood Oxygenation	↑

CO₂ stress:

Flow	↑↑
CMRO ₂	→
Blood Oxygenation	↑↑

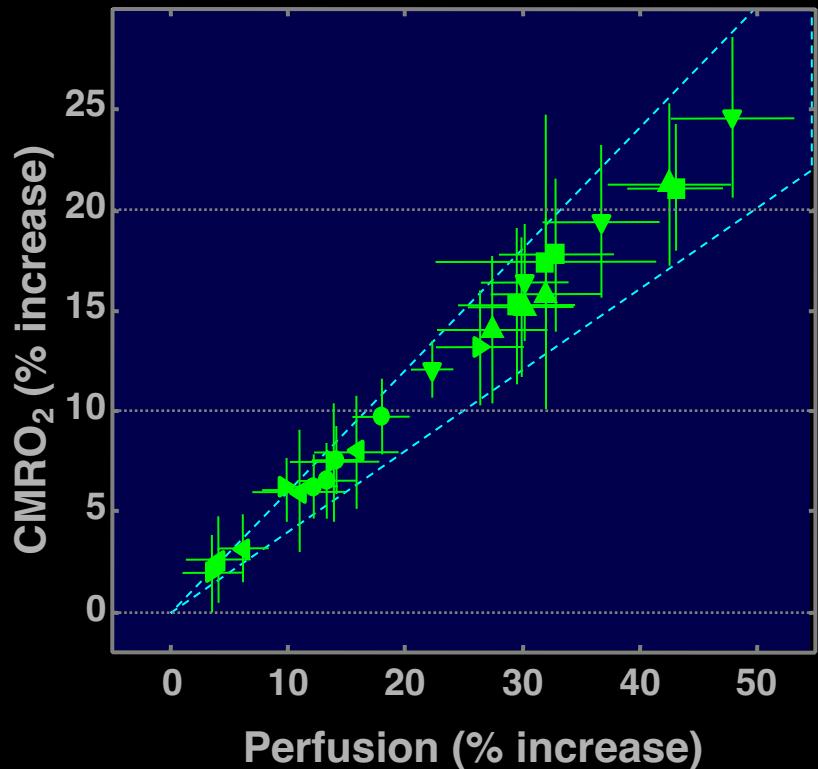
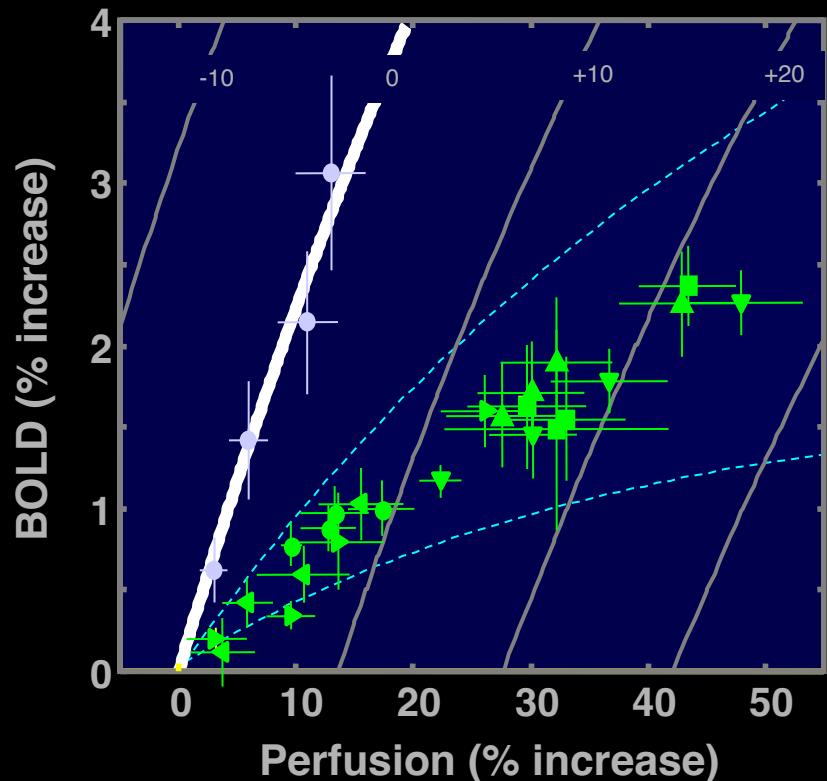
CMRO₂-related BOLD signal deficit:



Simultaneous Perfusion and BOLD imaging
during graded visual activation and hypercapnia

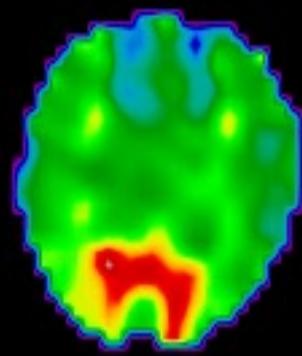
N=12

CBF-CMRO₂ coupling

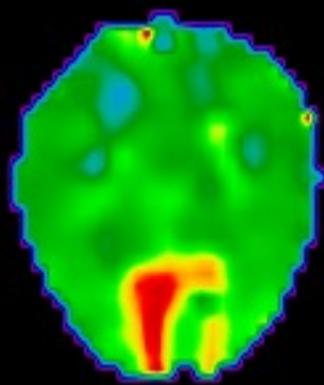


Characterizing Activation-induced CMRO₂ changes using calibration with hypercapnia

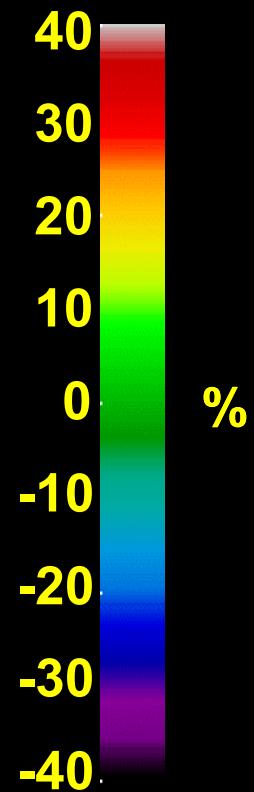
Computed CMRO₂ Changes



Subject 1



Subject 2



%

Variables to Optimize

- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

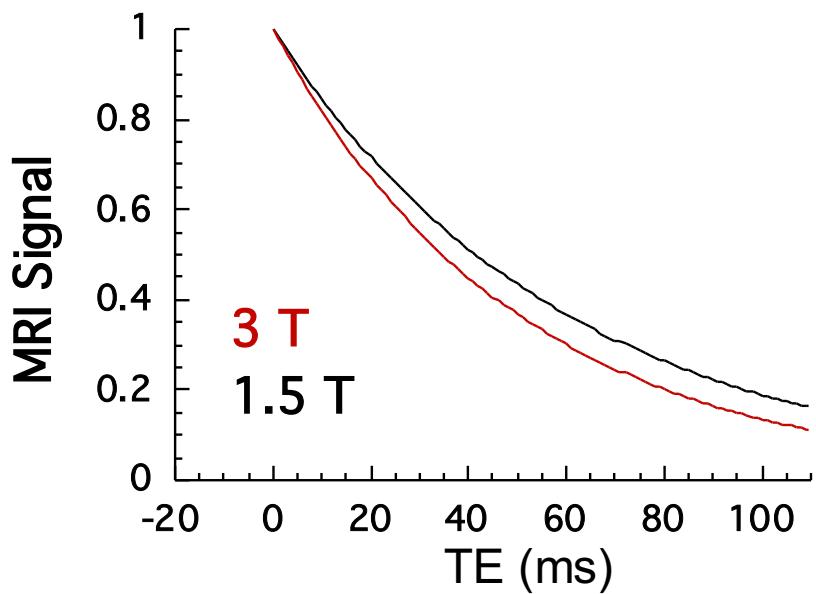
Sensitivity

- Optimizing fMRI Contrast
- Maximizing Signal
- Reducing Physiologic Fluctuations
- Minimizing Temporal Artifacts

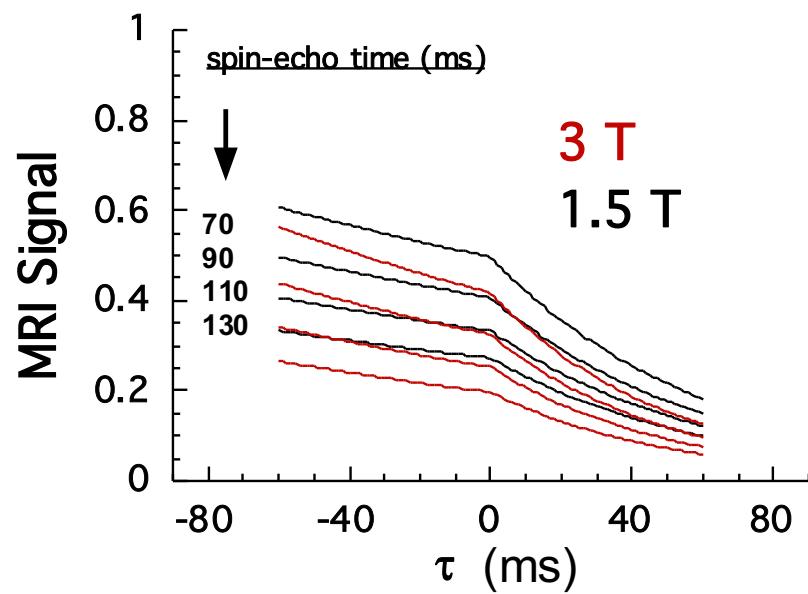
Optimizing fMRI Contrast

- Increase field strength
- Adjust pulse sequence timing ($TE \approx T2^*$)
- Adjust voxel volume (\approx activation volume)

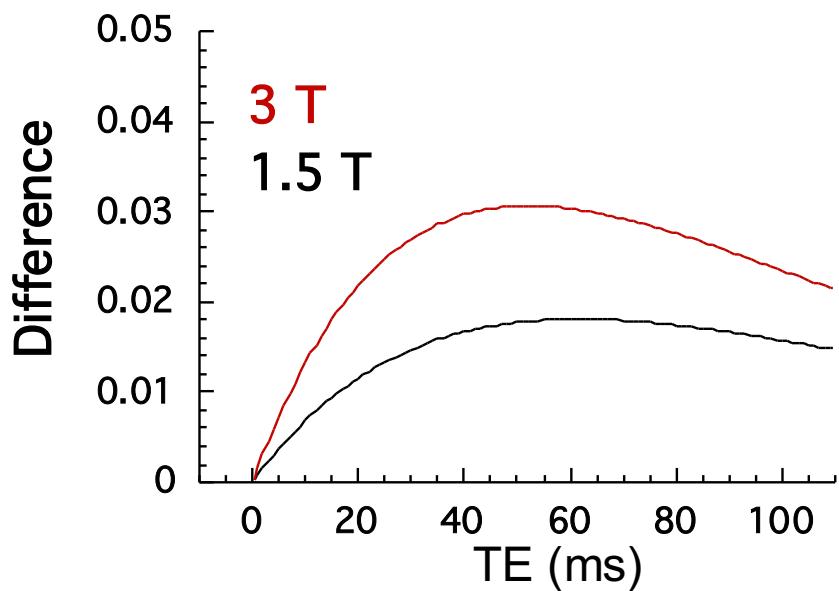
Gradient - Echo



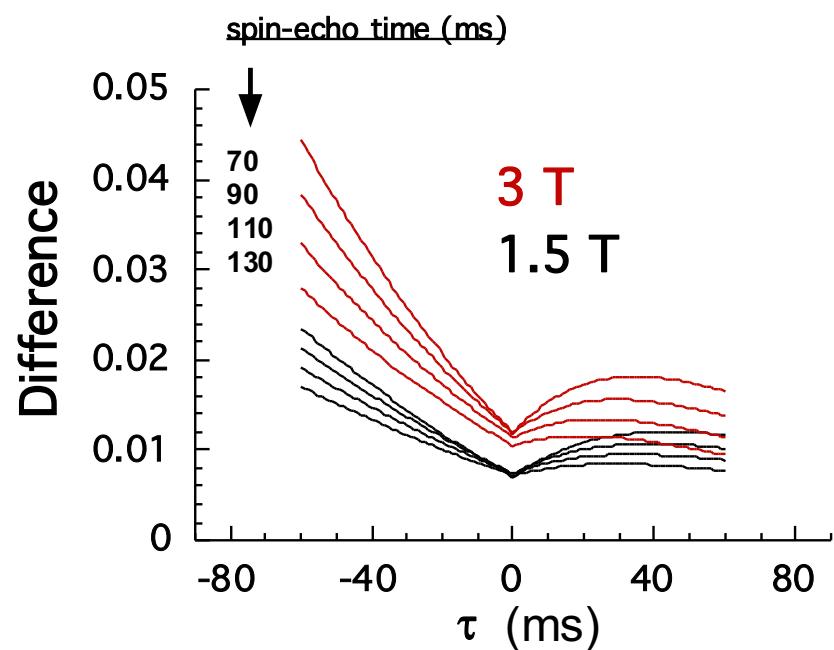
Asymmetric Spin - Echo



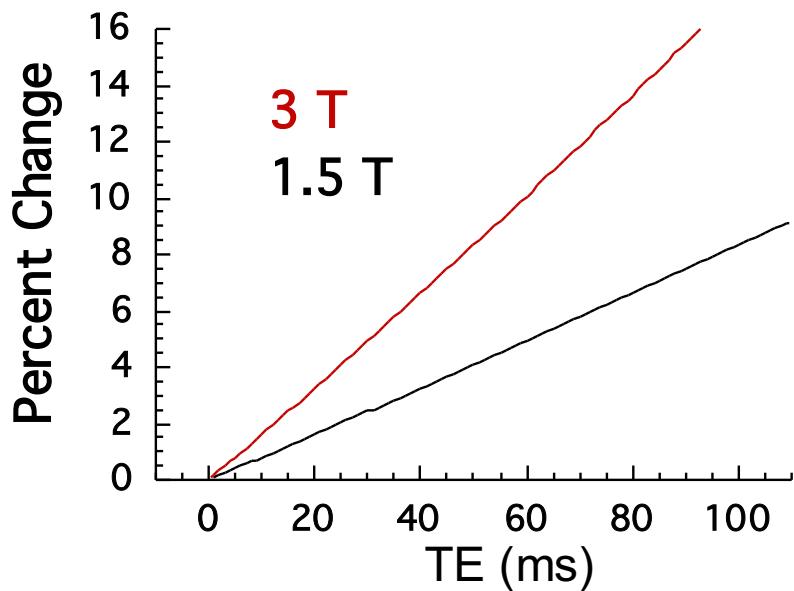
Gradient - Echo



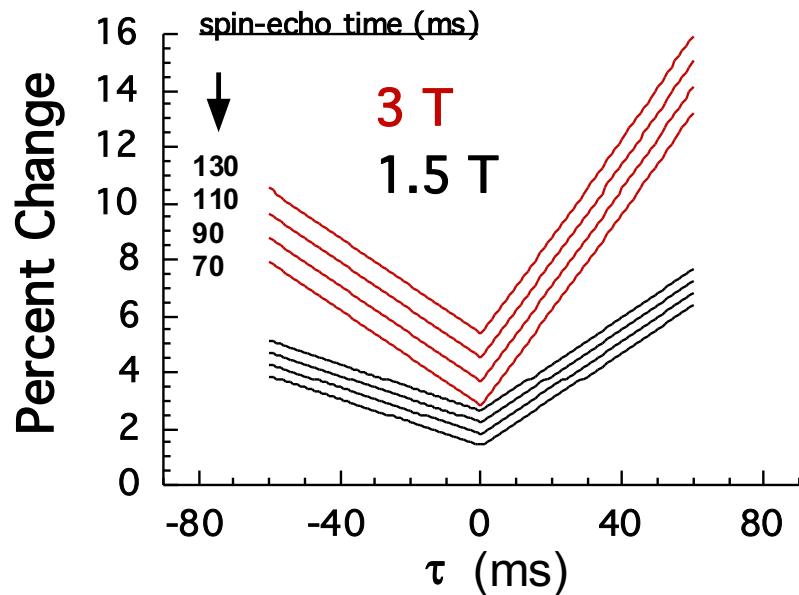
Asymmetric Spin - Echo



Gradient - Echo



Asymmetric Spin - Echo



Maximizing Signal

- Higher Bo Field
- Radio frequency Coils
- Choice of repetition time (TR)
- Voxel volume

Physiologic Fluctuations

Cardiac 0.6 to 1.2 Hz

Respiratory 0.1 to 0.2 Hz

Low Frequency 0.0 to 0.1 Hz

0.25 Hz Breathing at 1.5T

Power Spectra

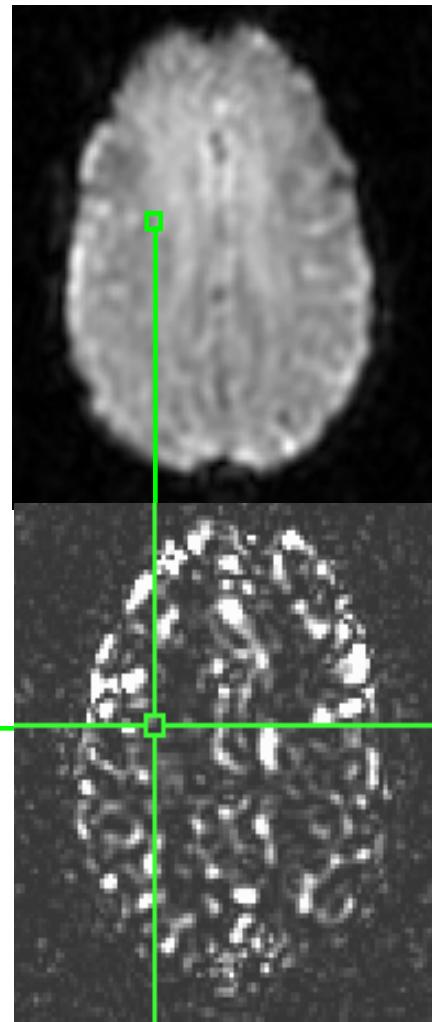
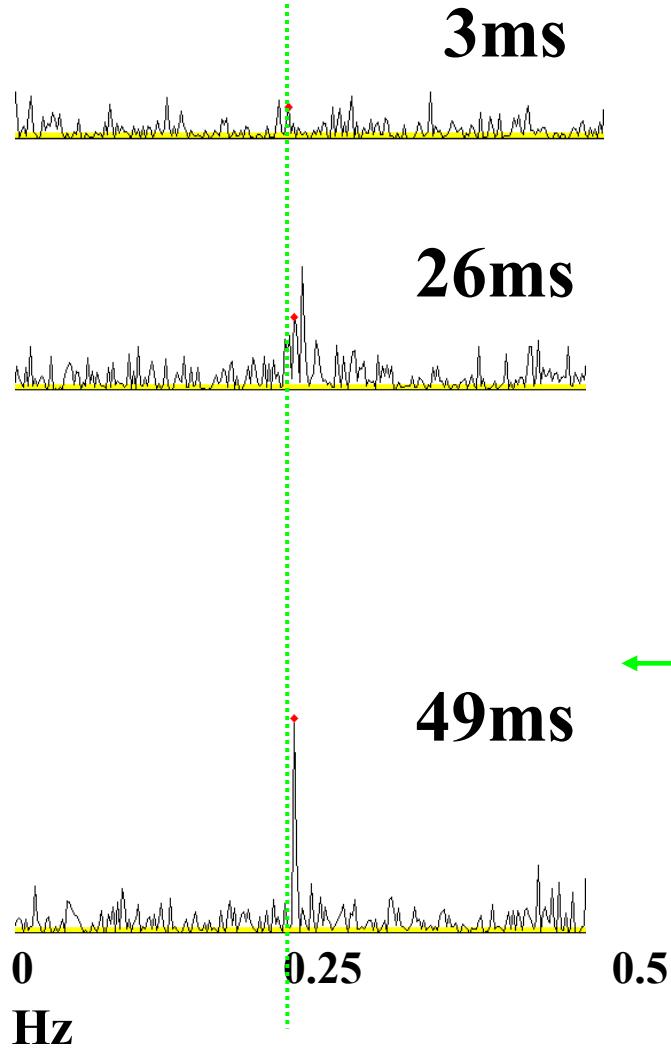


Image Respiration map

0.68 Hz Cardiac rate at 3T

Power Spectra

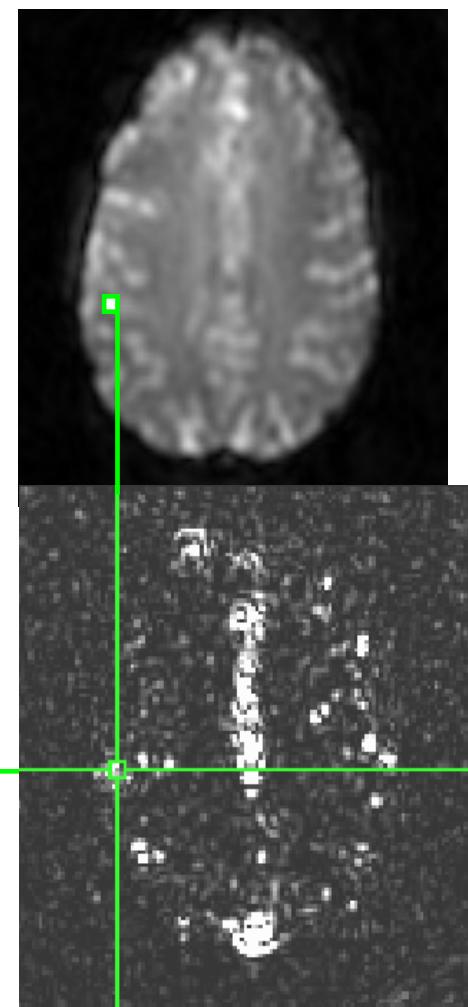
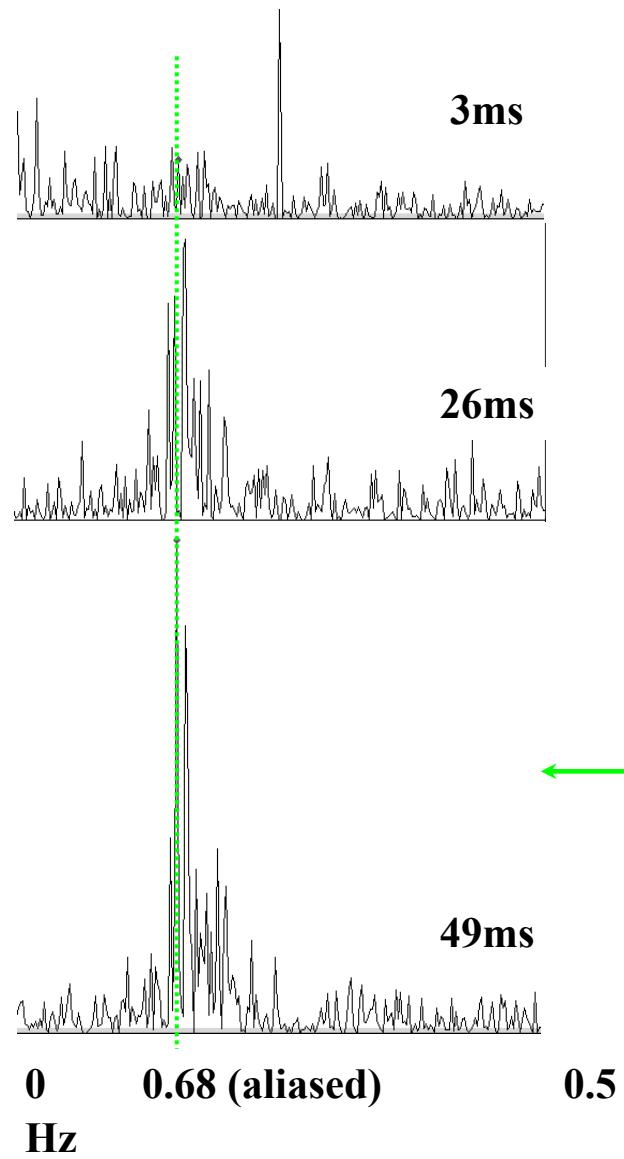
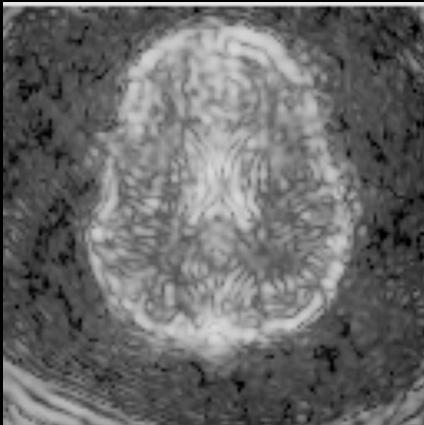


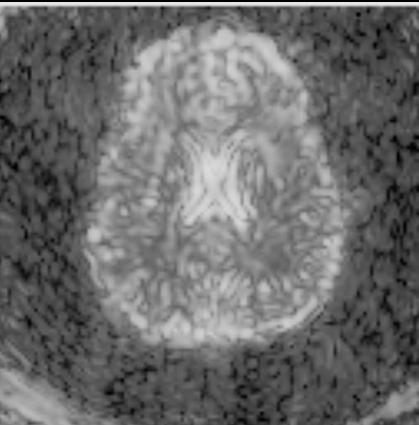
Image
Cardiac map

Temporal vs. Spatial SNR- 3T

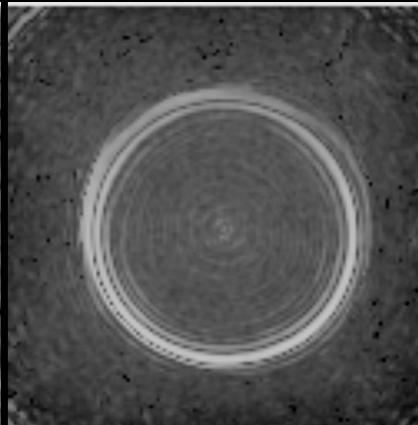
26ms



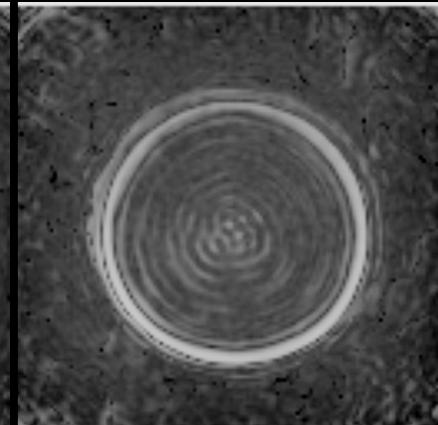
49ms



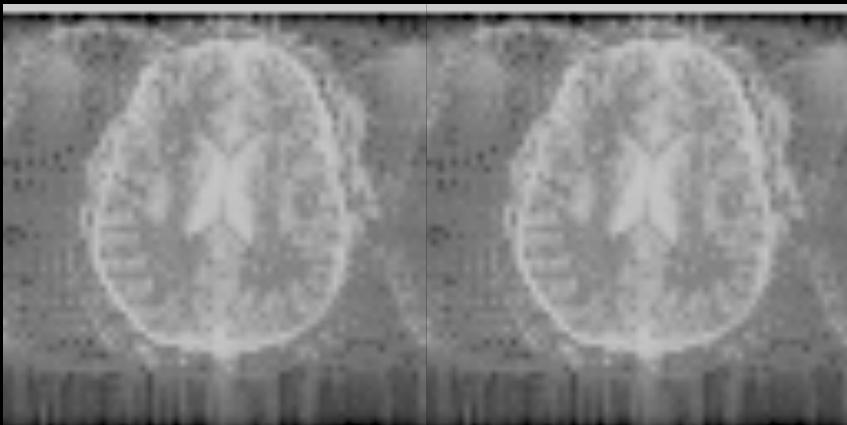
26ms



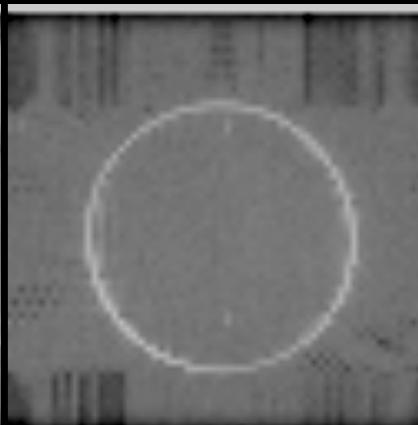
49ms



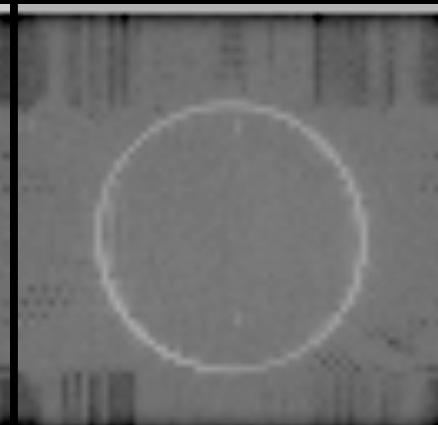
27ms



50ms



27ms



50ms

SPIRAL EPI

Reducing Physiologic Fluctuations

- Filtering
- Pulse sequence
 - single vs. multishot
 - strategies for multishot
- Gating with correction for variable TR

Temporal Artifacts

- System instabilities
- Motion
 - Drift
 - Stimulus correlated
 - Stimulus uncorrelated

Minimizing Temporal Artifacts

Recognize?

- Edge effects
- Shorter signal change latencies
- Unusually high signal changes
- External measuring devices

Correct?

- Image registration algorithms
- Orthogonalize to motion-related function (*cardiac, respiration, movement*)
- Navigator echo for k-space alignment
(for multishot techniques)
- Re-do scan

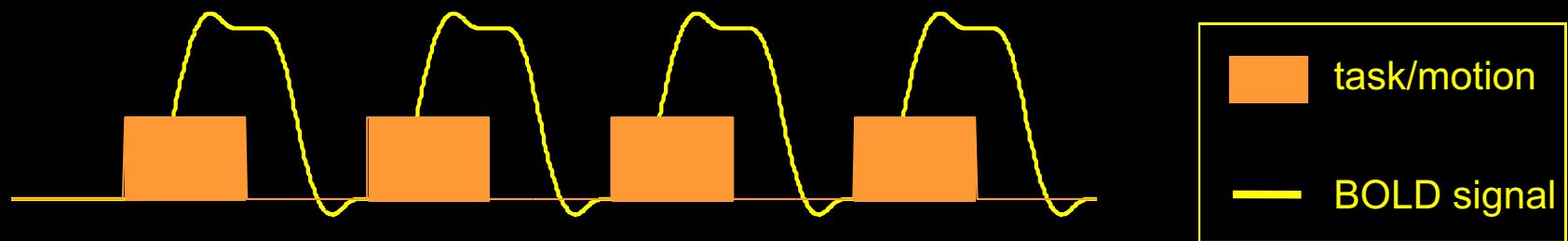
Bypass?

- Paradigm timing strategies..
- Gating (with T1-correction)

Suppress?

- Flatten image contrast
- Physical restraint
- Averaging, smoothing

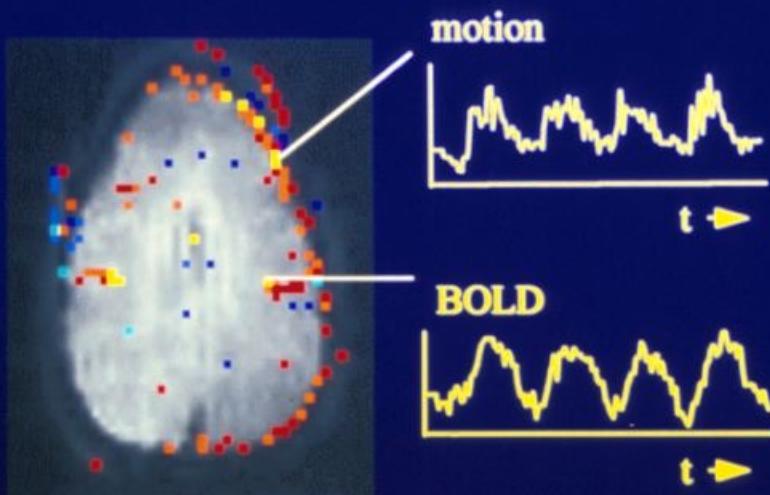
Block-trial



Single-trial (brief stimulus)

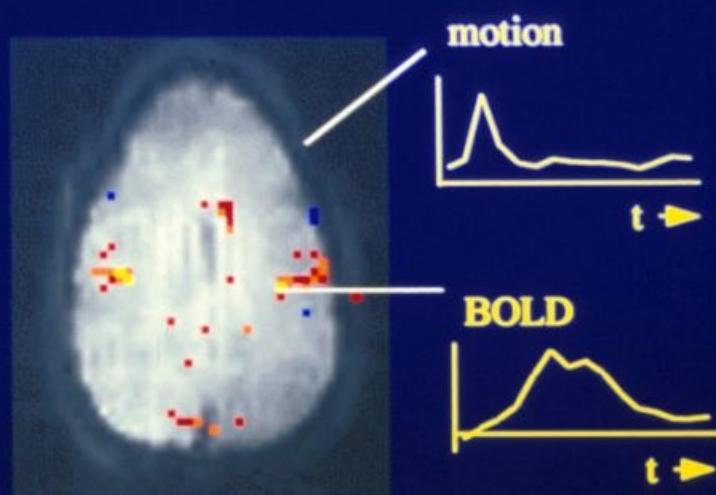


Motion-Decoupled fMRI: Functional MRI during overt word production



"block-trial" paradigm

Motion induced signal changes resemble functional (BOLD) signal changes



"single-trial" paradigm

Motion induced and BOLD signal changes are separated in time

R.M. Birn, et al.

Overt Word Production



2

3

4

5



6

7

8

9



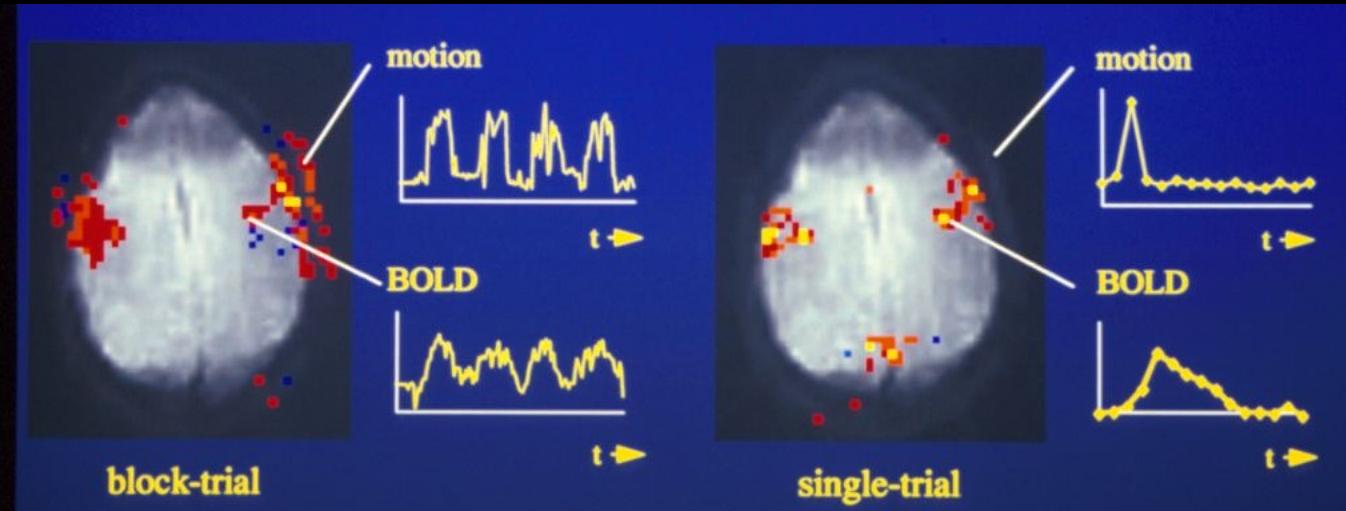
10

11

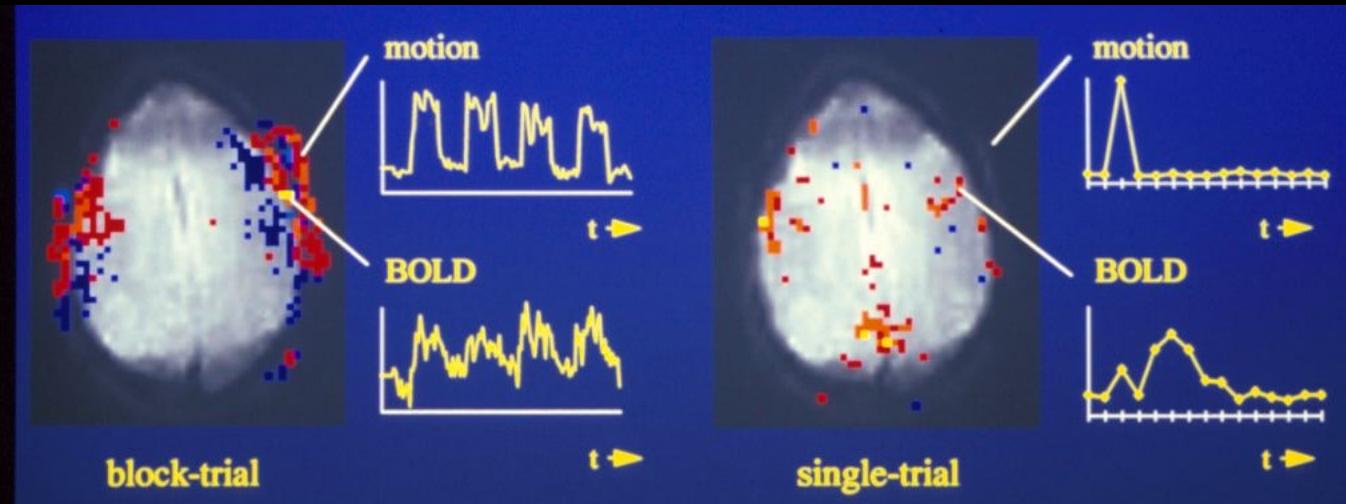
12

13

Tongue Movement



Jaw Clenching



Variables to Optimize

- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

Speed

- Rapid imaging techniques:

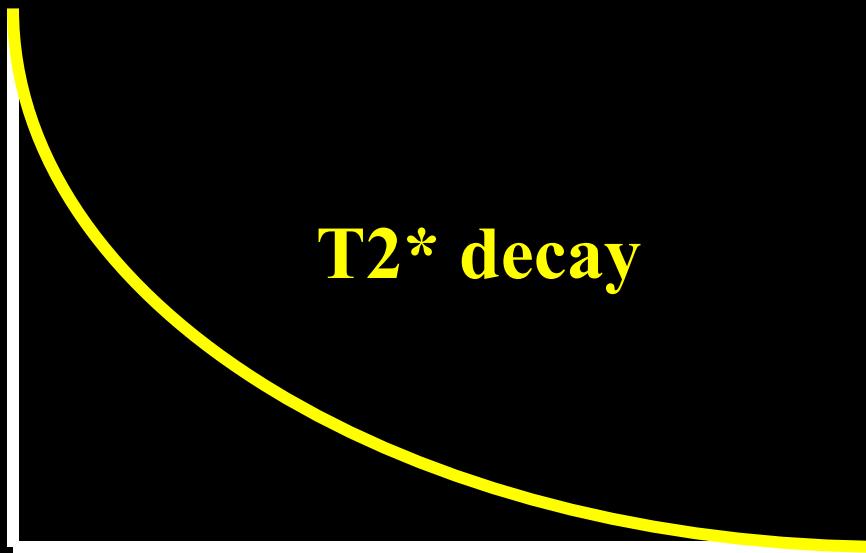
- Single shot imaging
 - TR vs. Brain coverage:

$$\text{min TR} = (\text{time/slice}) \times \text{number of slices in volume}$$

- Hemodynamic Issues

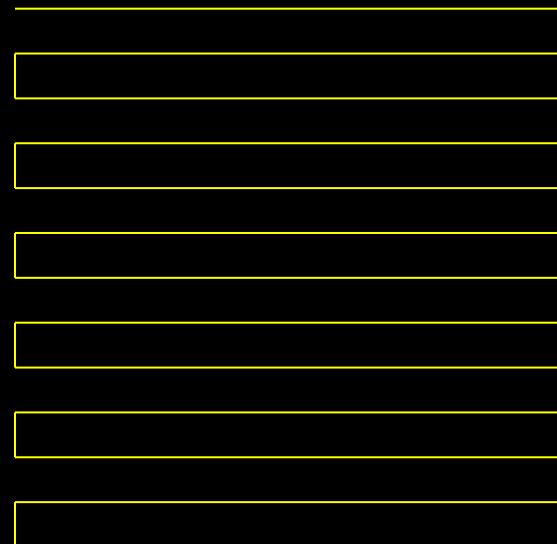
- Paradigm timing
 - Event related fMRI
 - Timing modulation

Single Shot Imaging

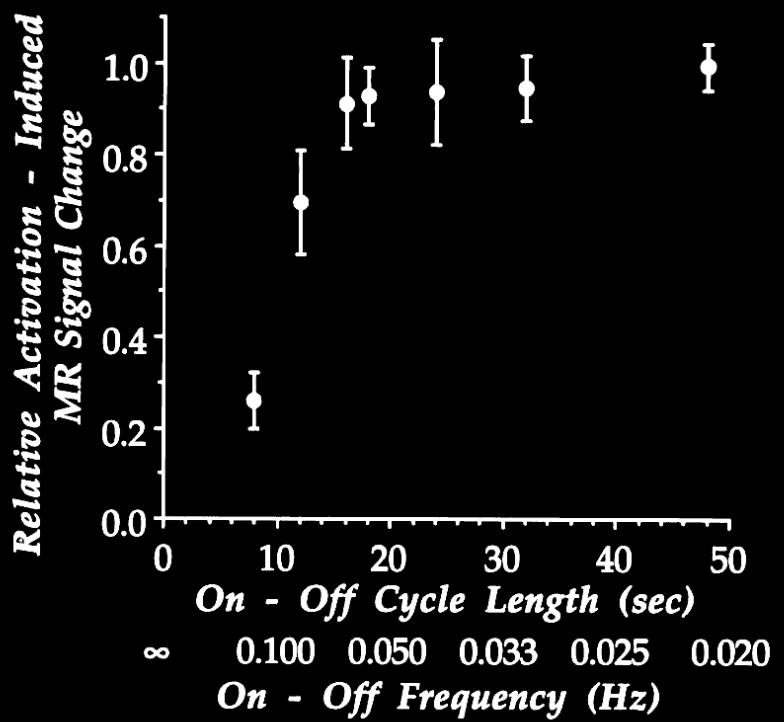
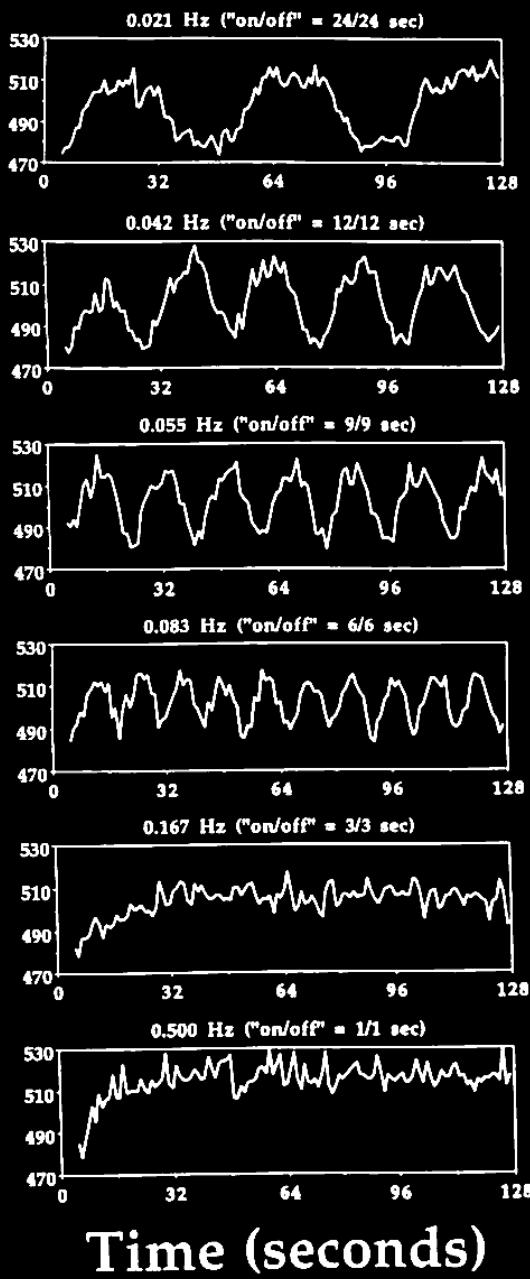


EPI Readout Window

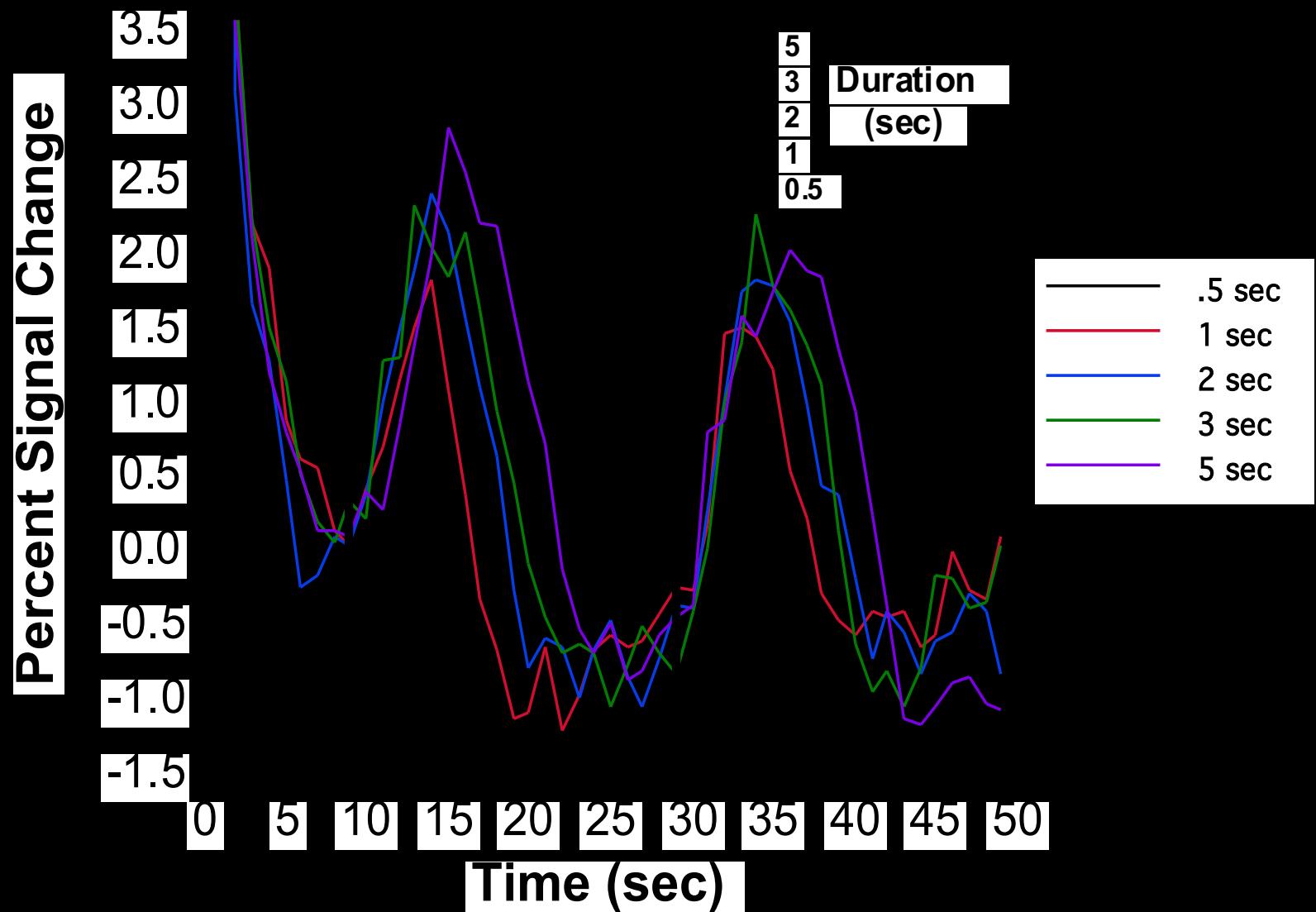
≈ 20 to 40 ms

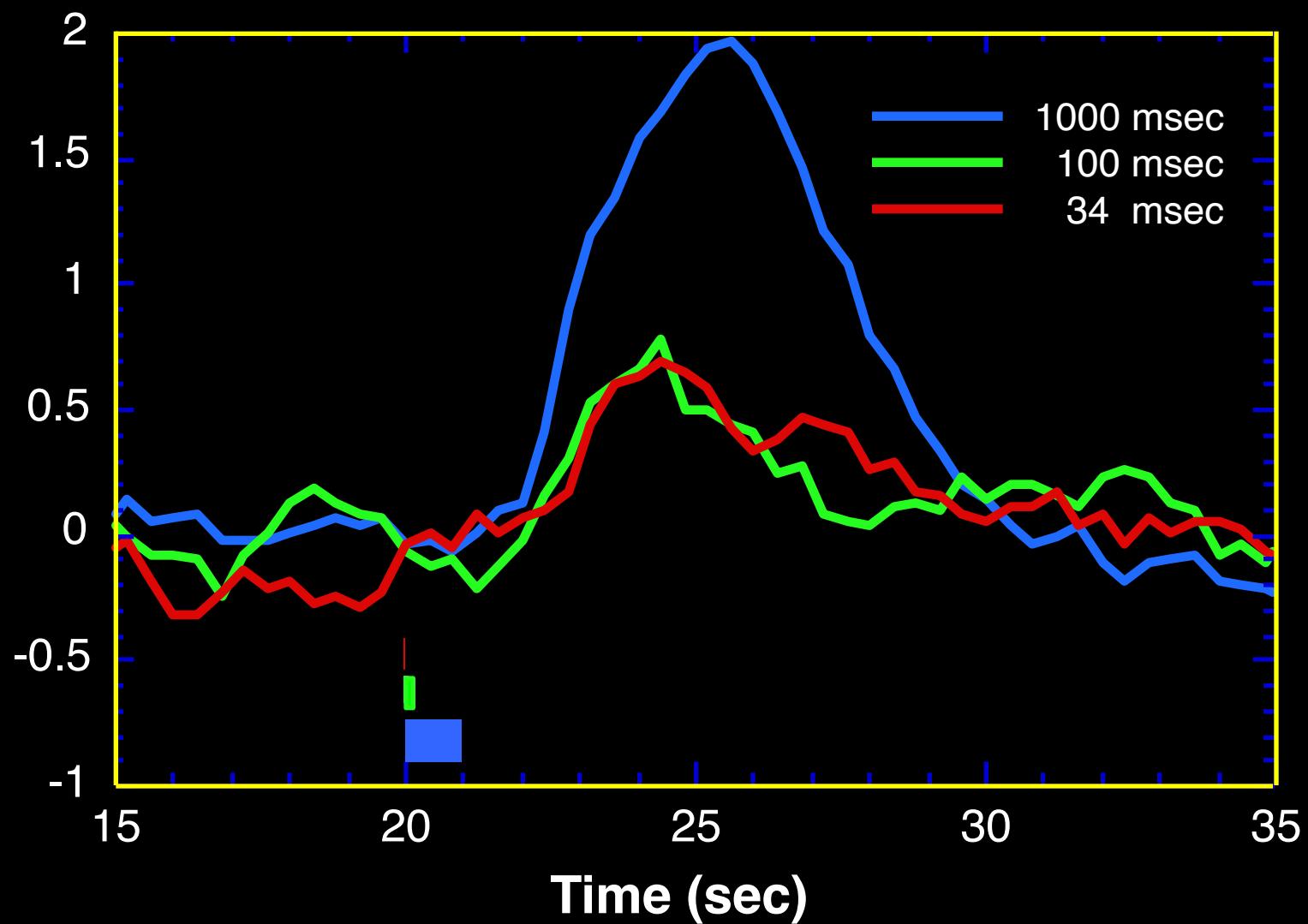


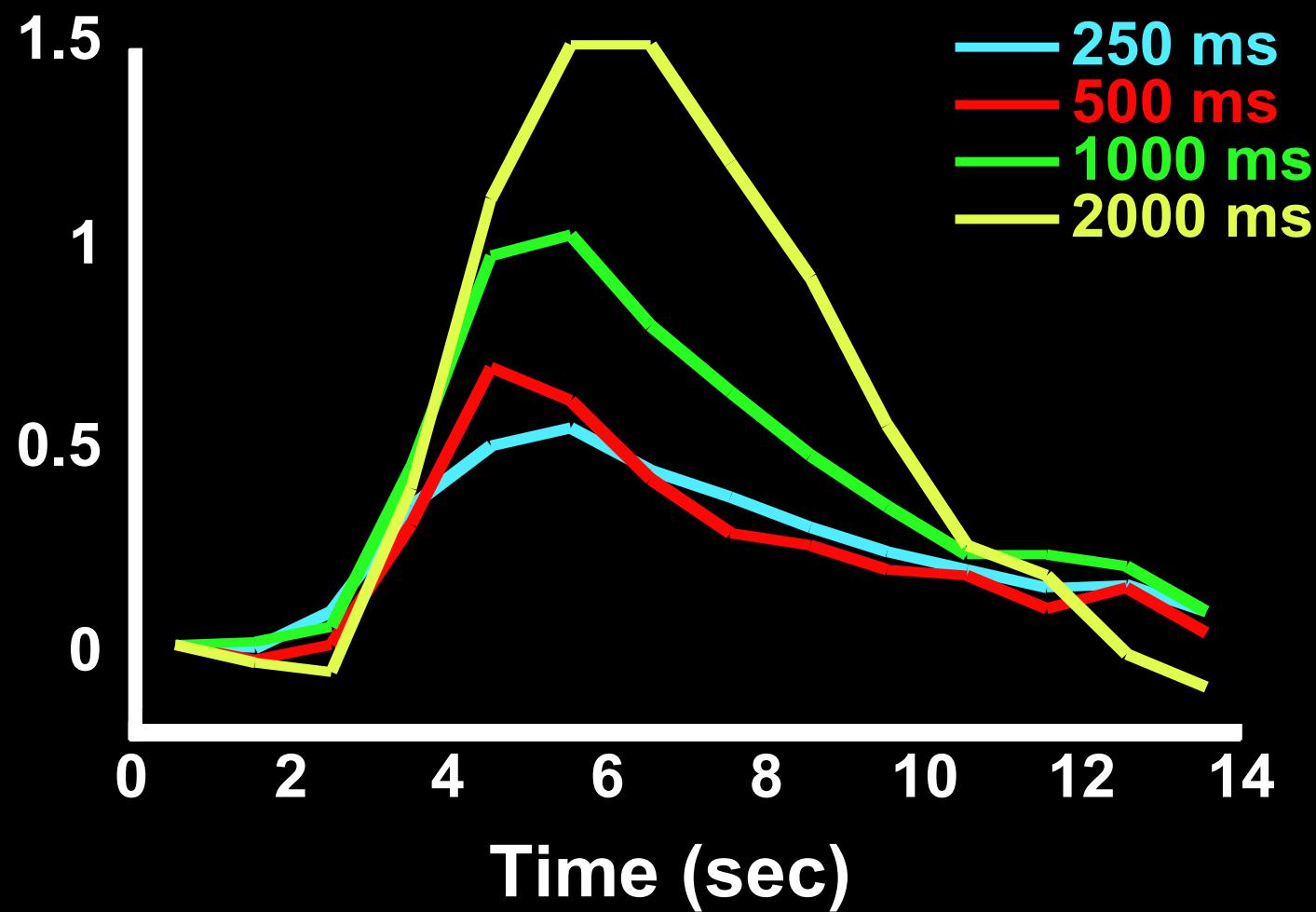
MRI Signal



Motor Cortex

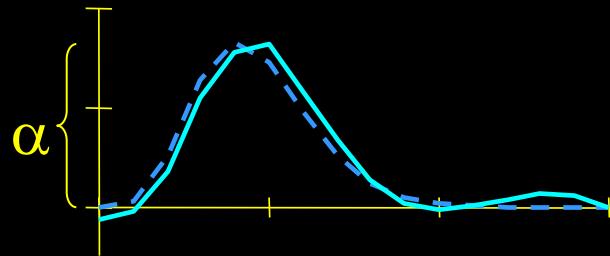






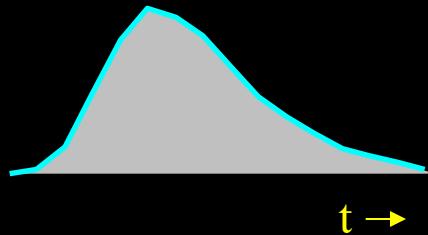
Compute nonlinearity (*for each voxel*)

- Amplitude of Response



Fit ideal (linear) to response

- Area under response / Stimulus Duration

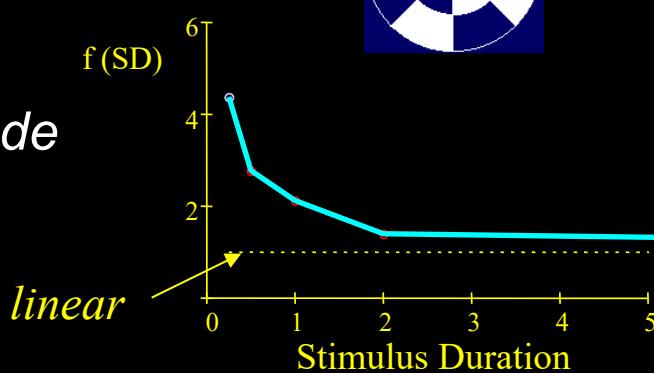


Output Area / Input Area

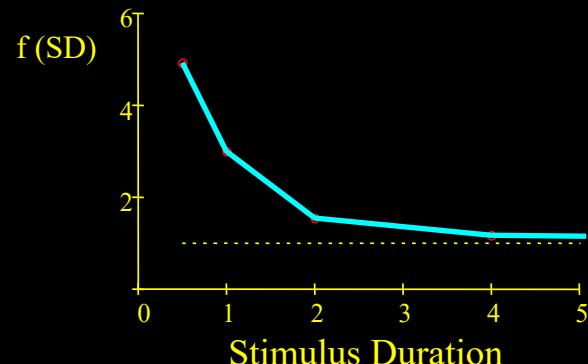
Nonlinearity

Visual

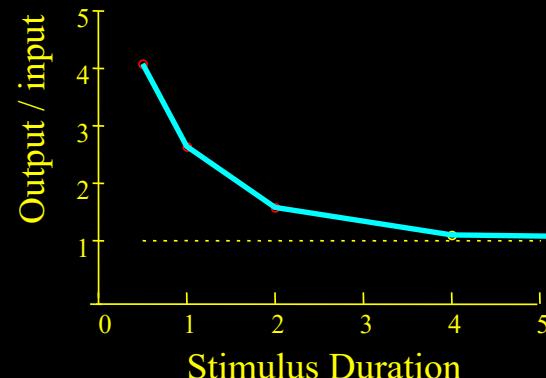
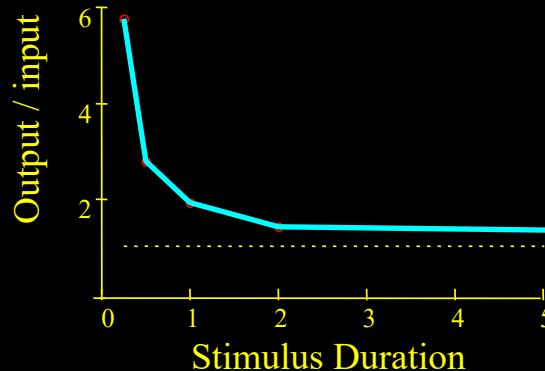
Magnitude



Motor

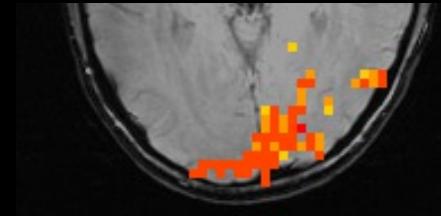
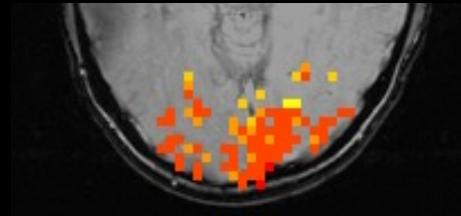
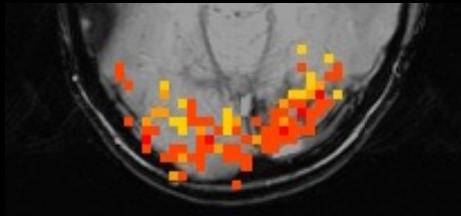


Area

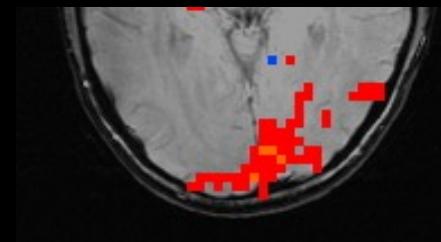
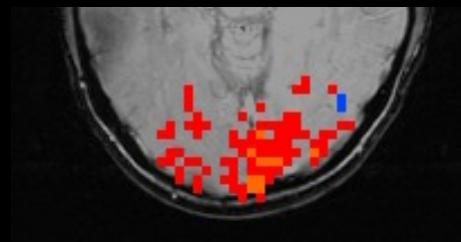
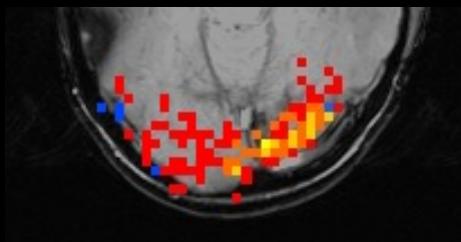


Results – visual task

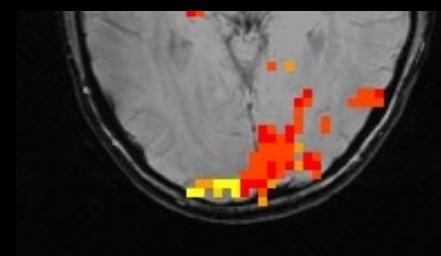
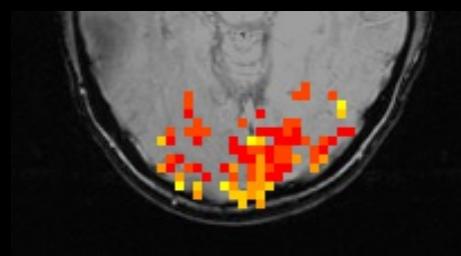
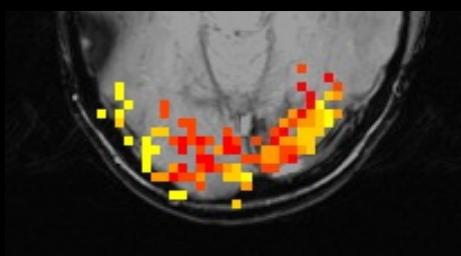
Nonlinearity



Magnitude

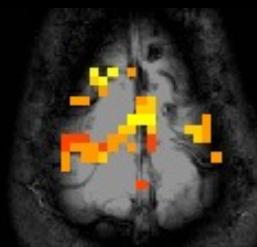
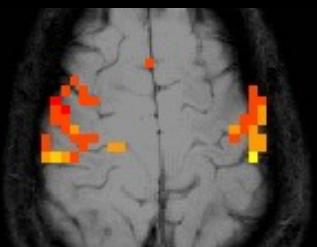
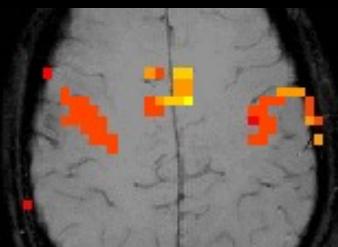


Latency

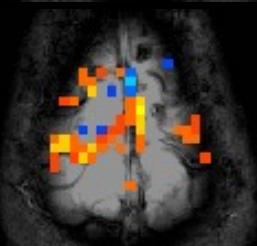
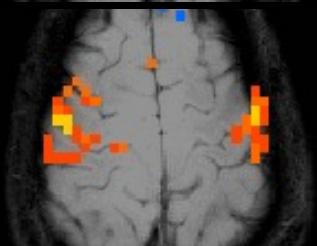
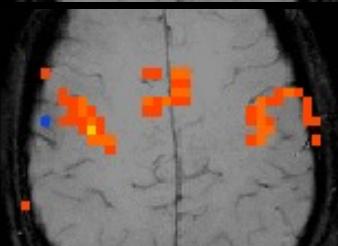


Results – motor task

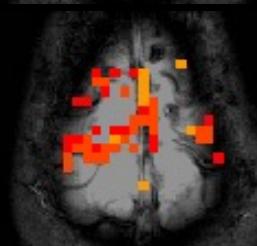
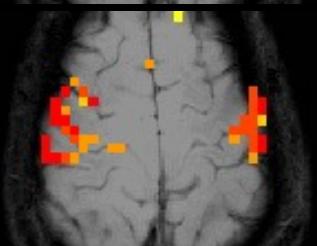
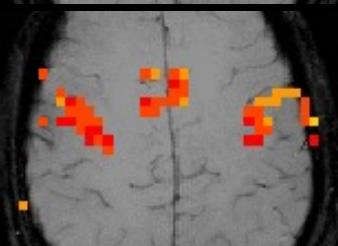
Nonlinearity



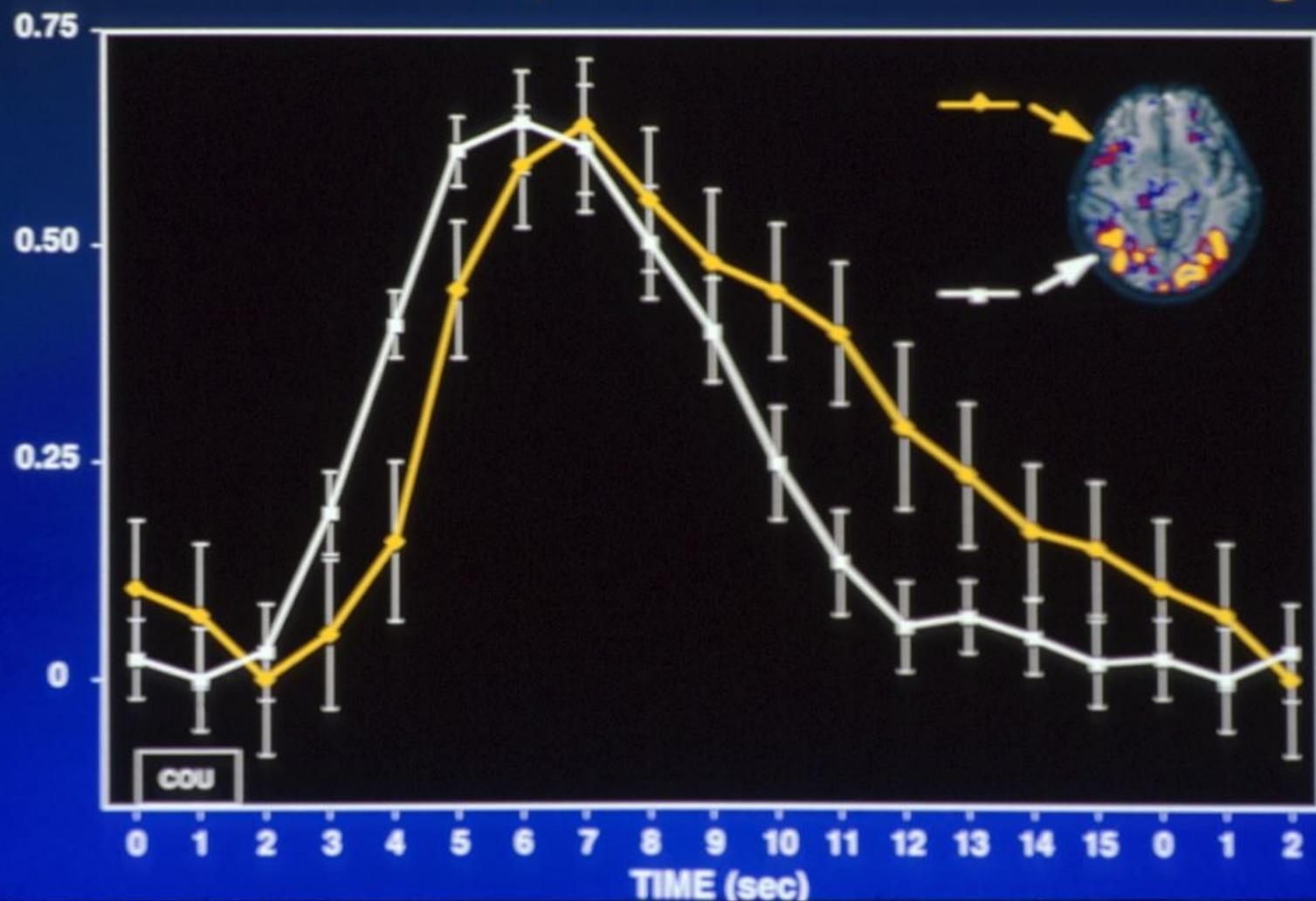
Magnitude



Latency



Time Course Comparison Across Brain Regions



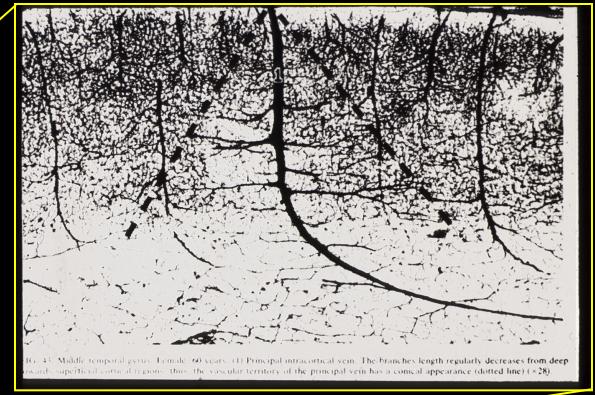
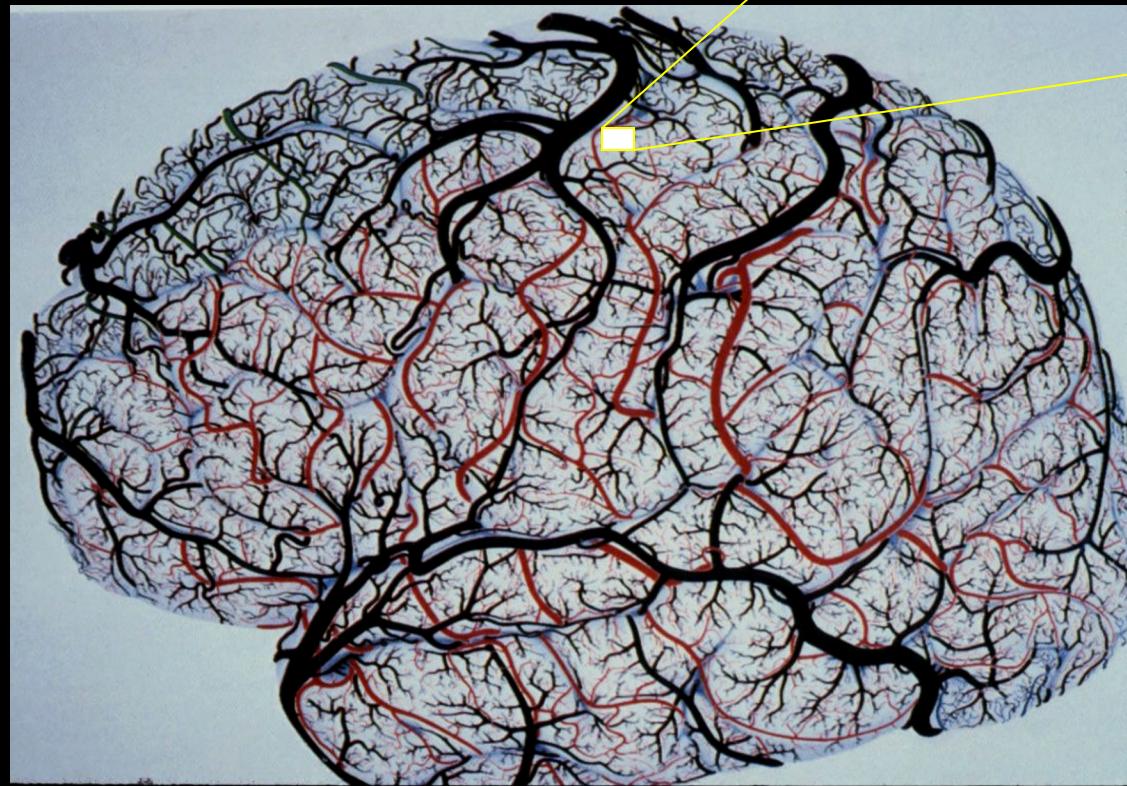
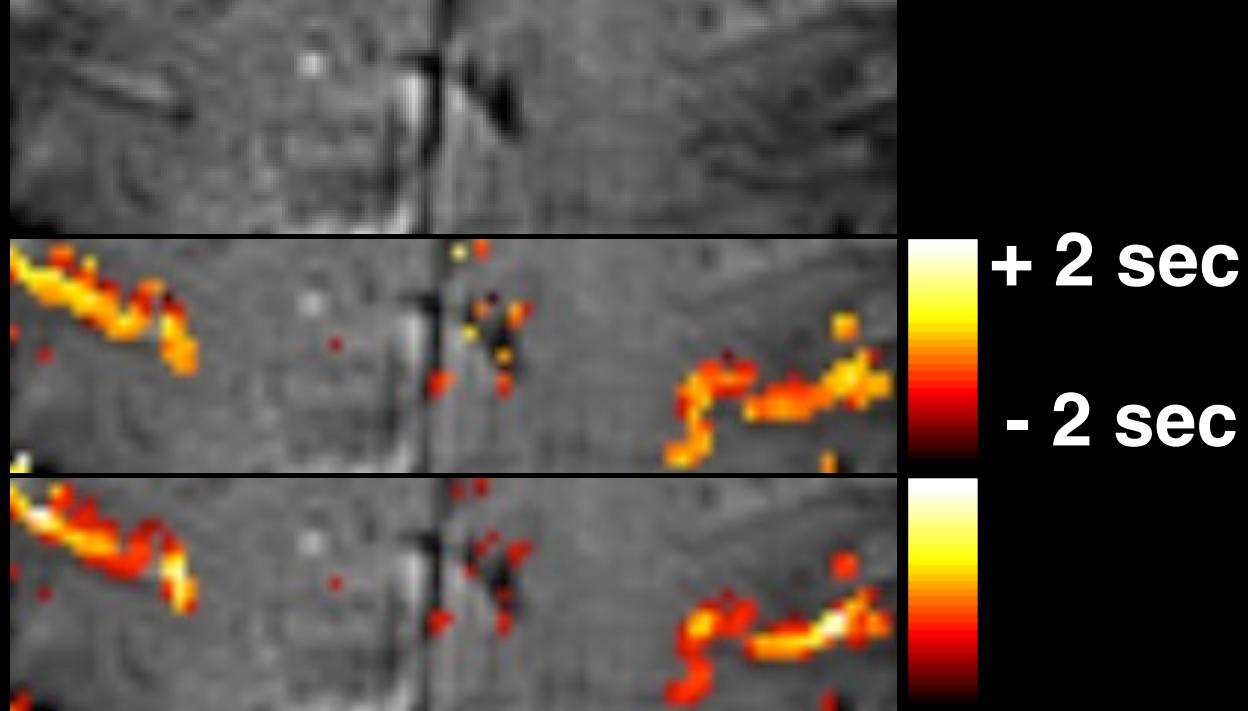
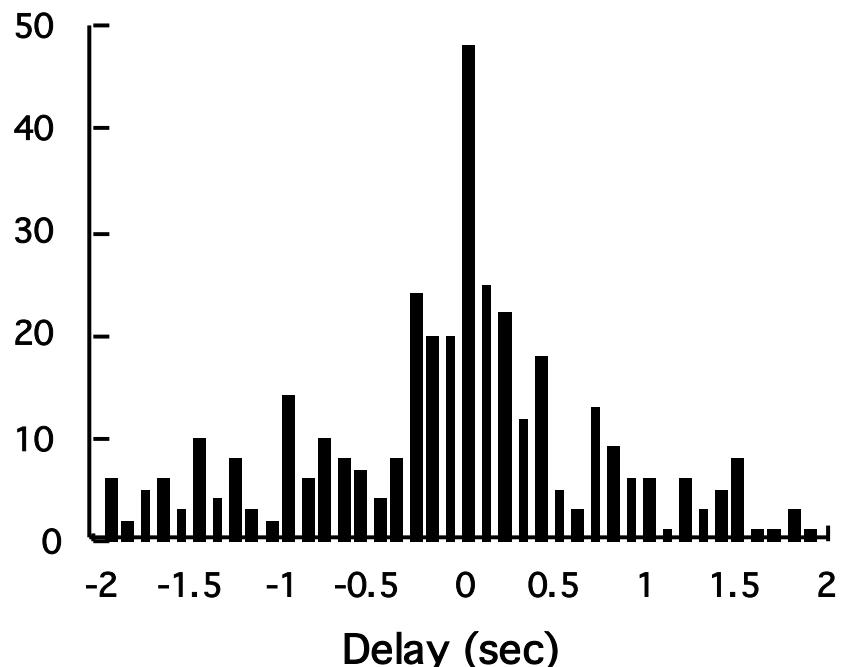
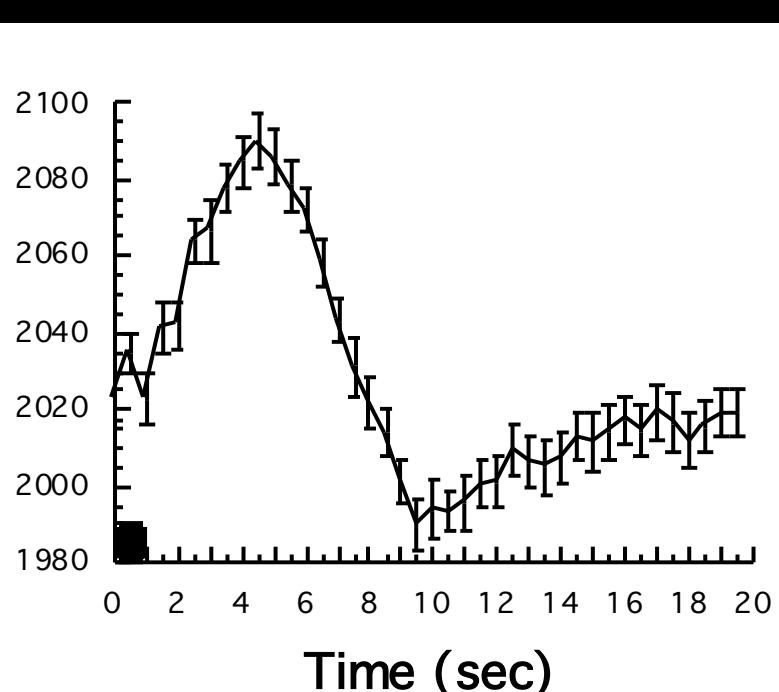


Fig. 4. Middle temporal gyrus. Female, 60 years. (1) Principal intracortical vein. The branches length regularly decreases from deep to superficial cortical regions; thus, the vascular territory of the principal vein has a conical appearance (dotted line) ($\times 28$)

Latency

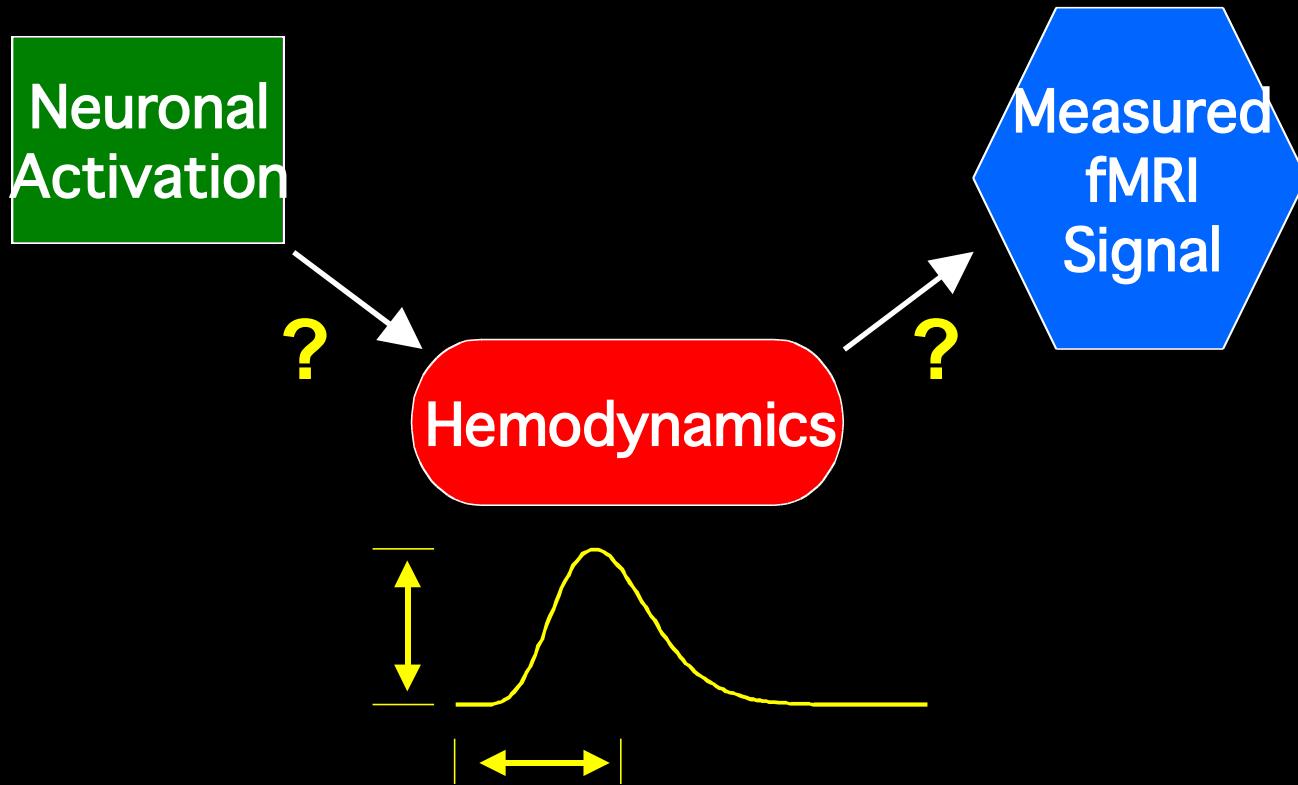


Magnitude



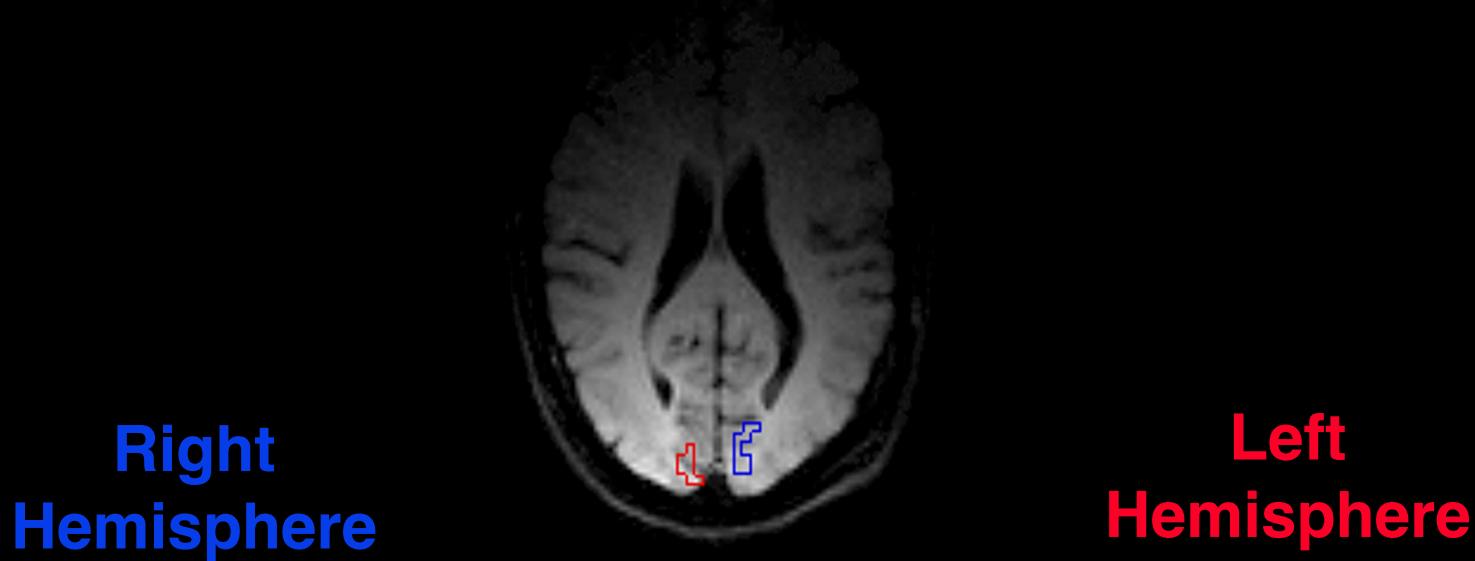
Temporal Normalization

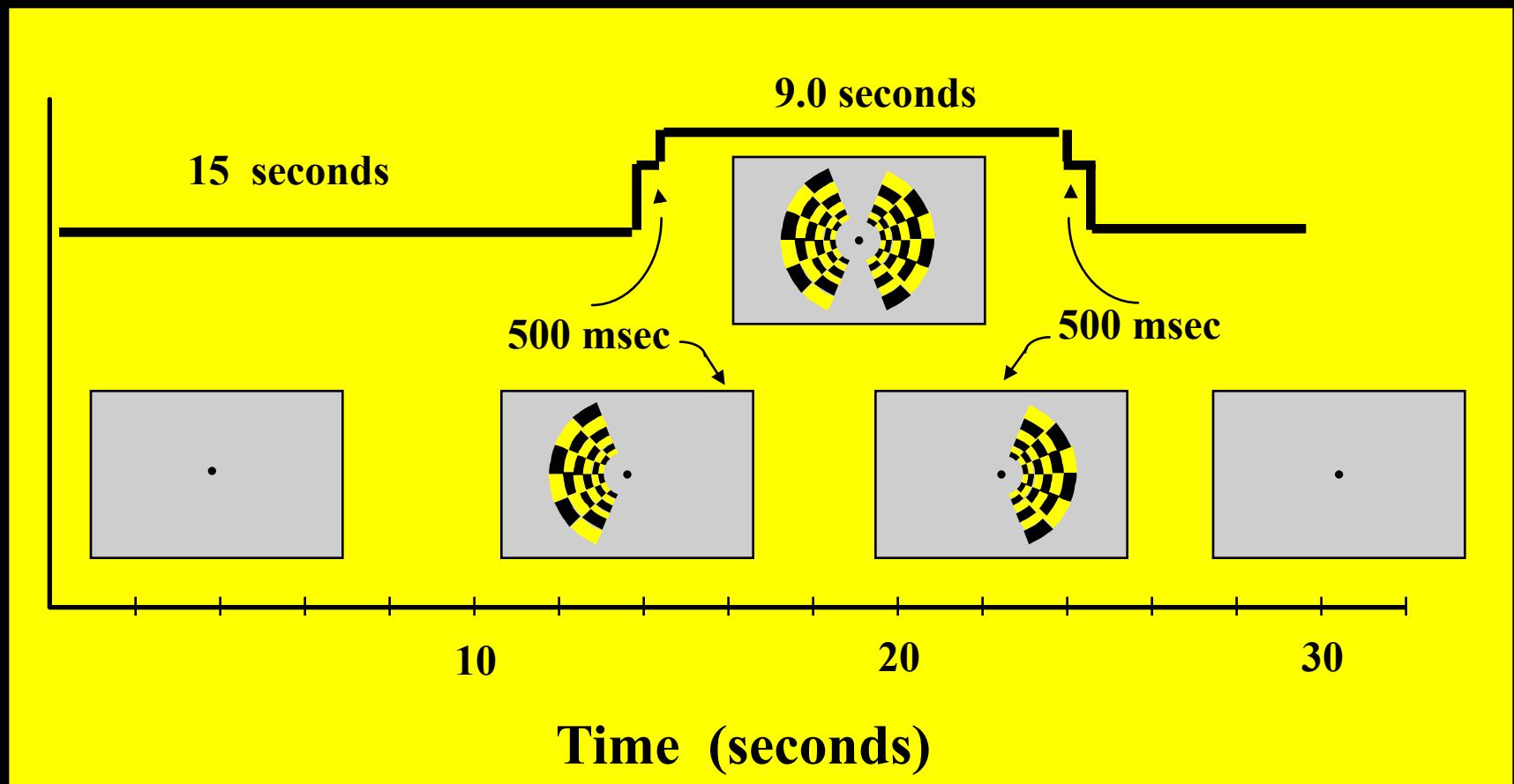
Relative Timing



Physiologic Factors

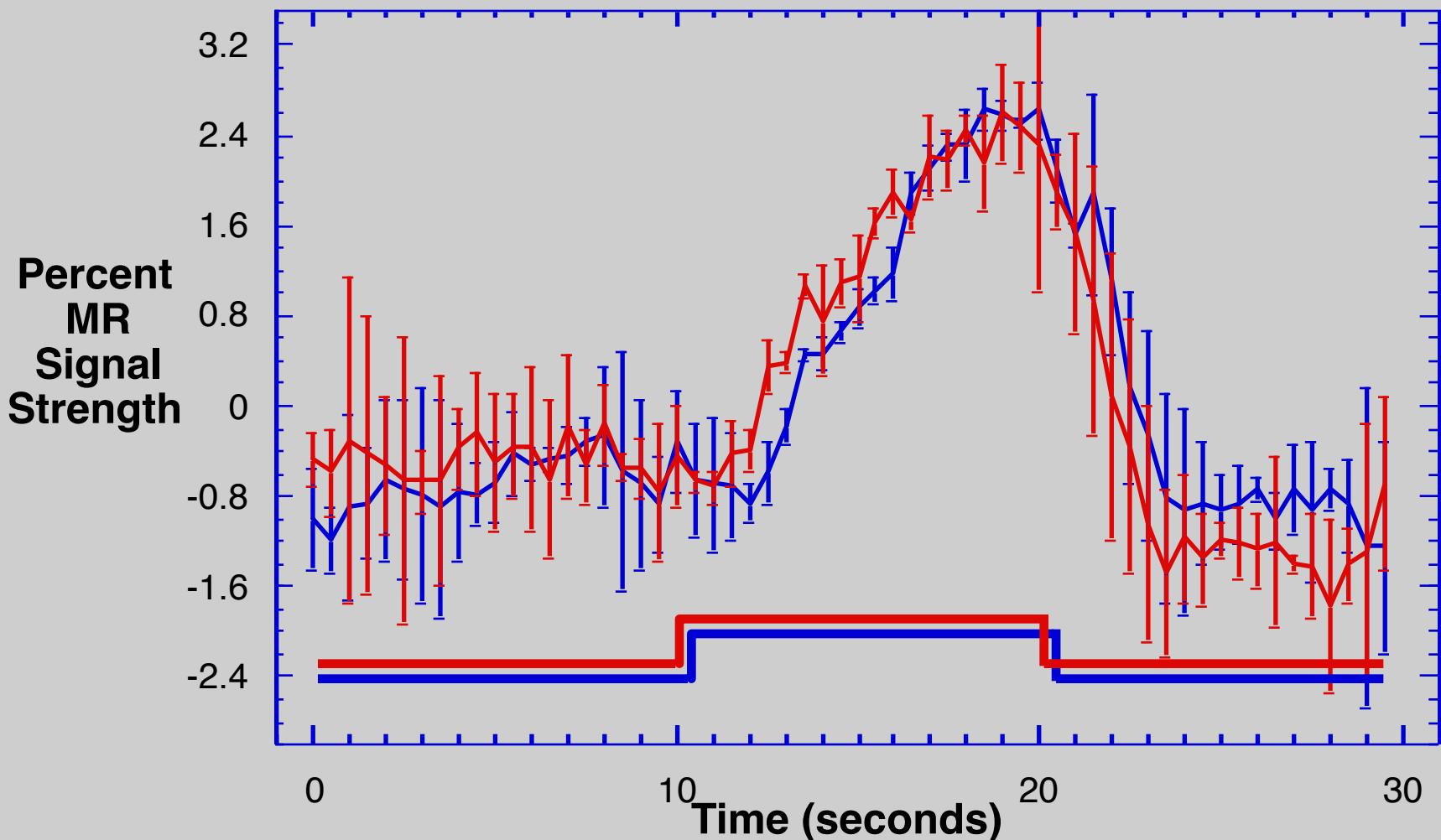
Regions of Interest Used for Hemi-Field Experiment



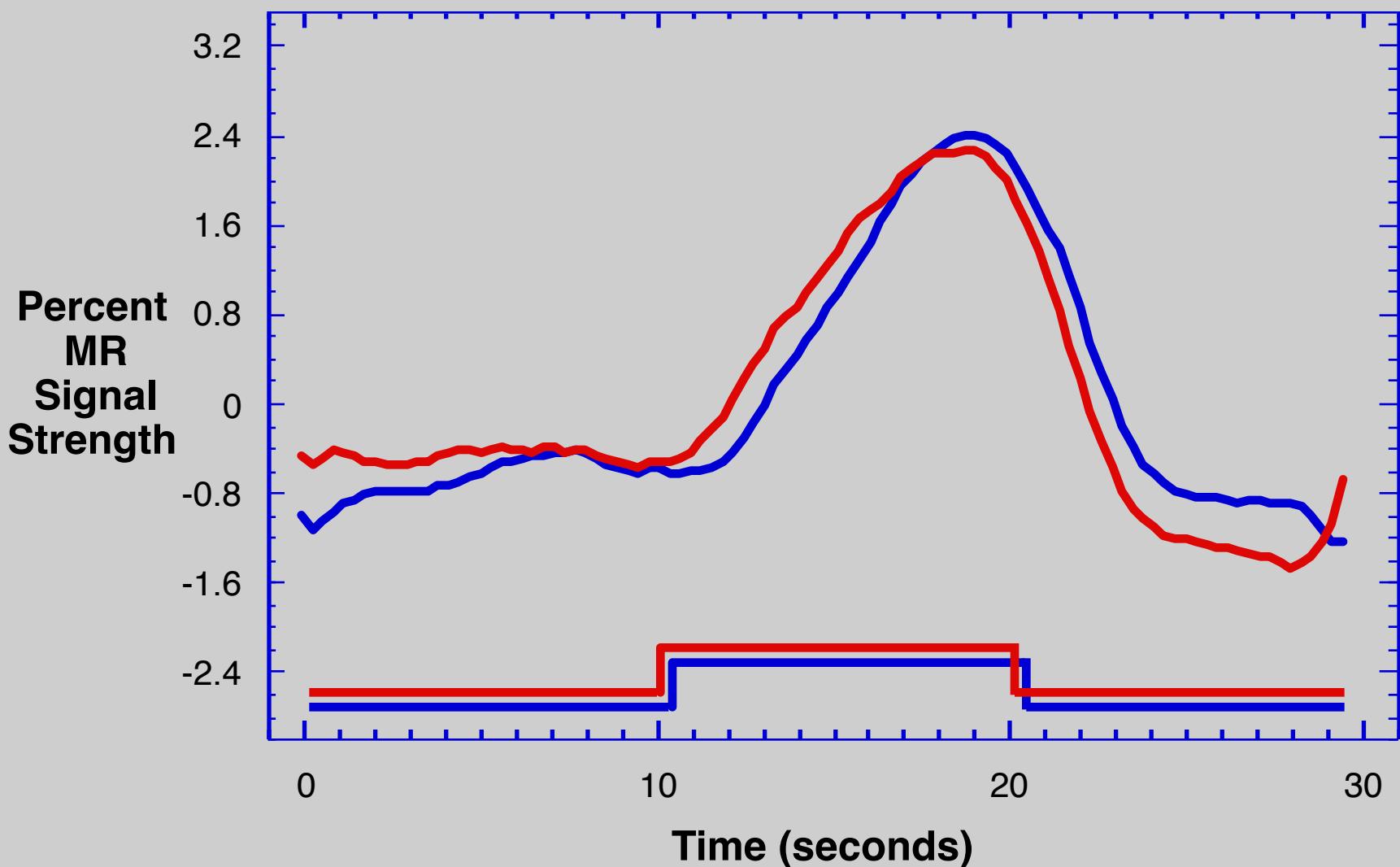


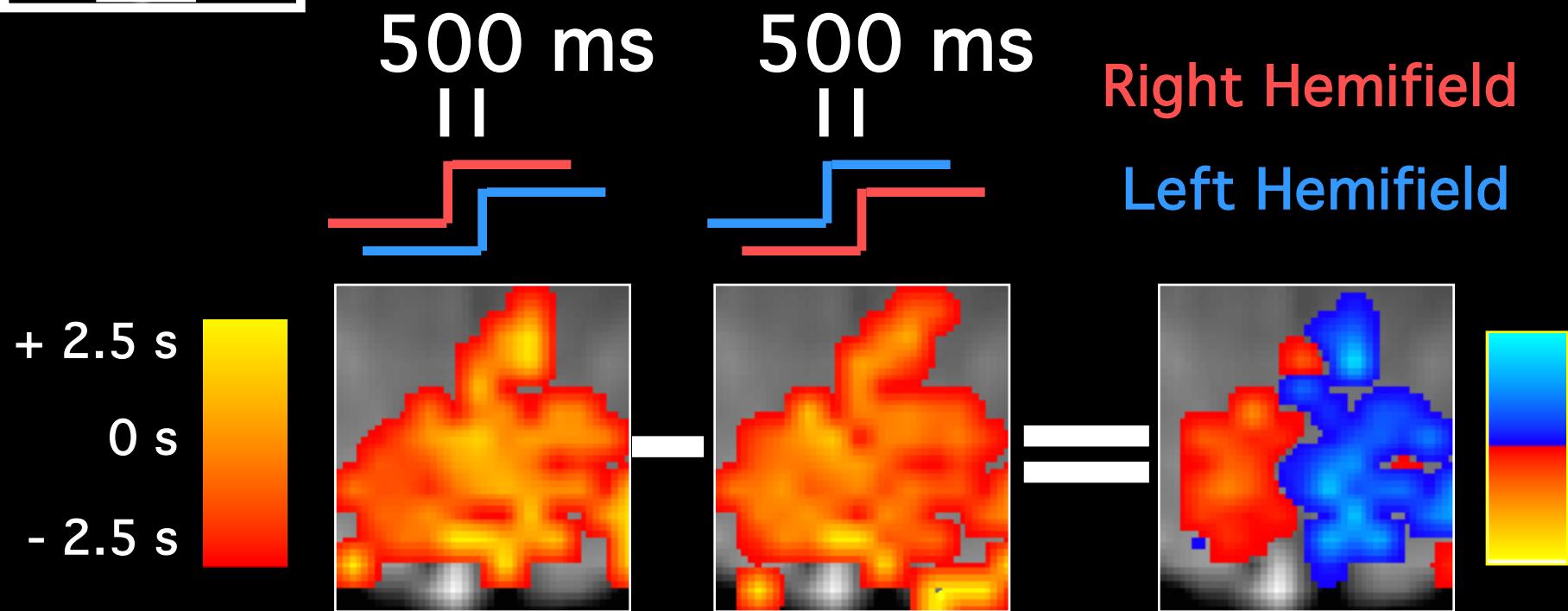
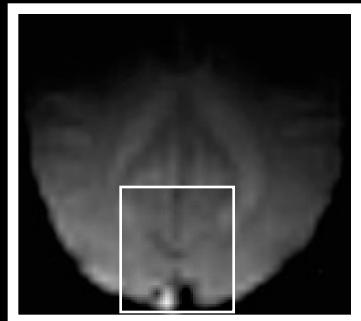
Hemi-field with 500 msec asynchrony

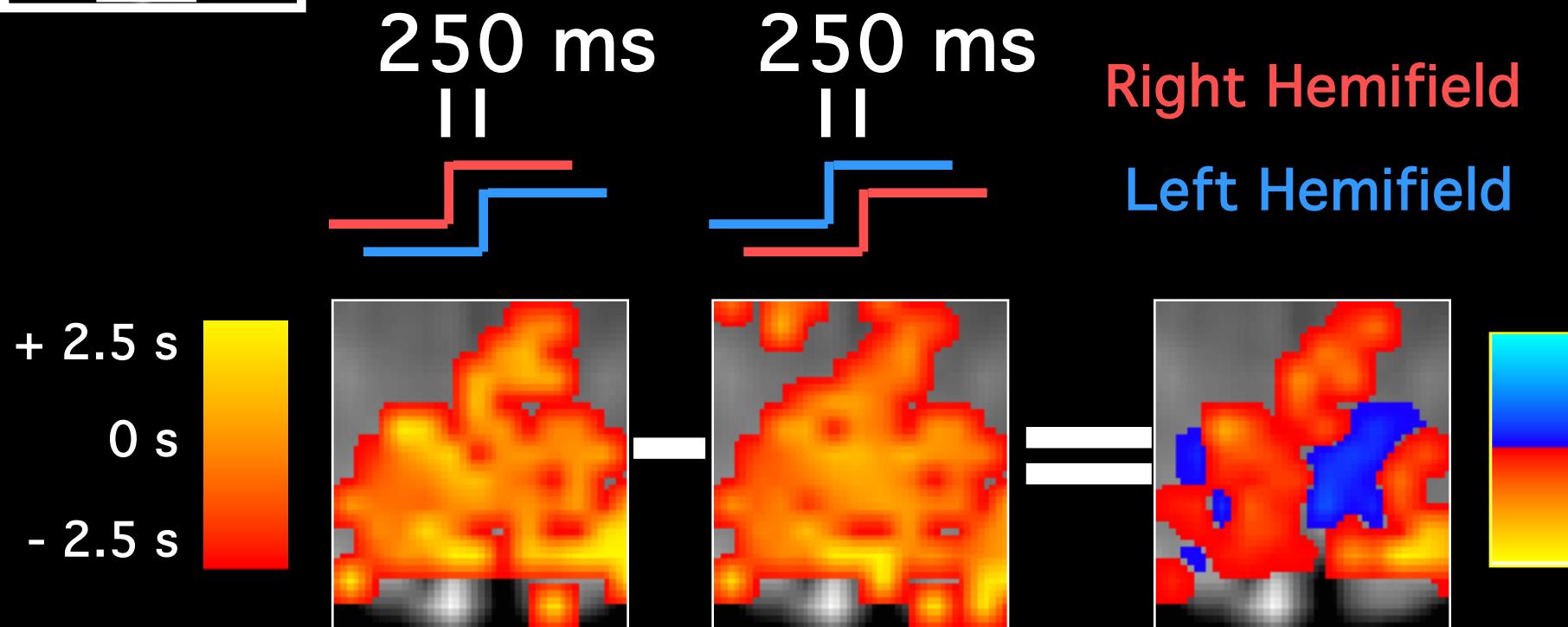
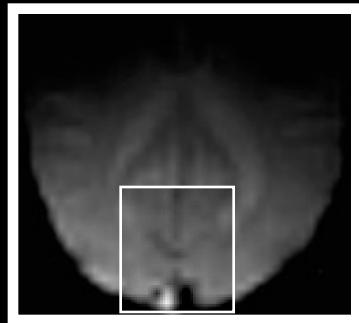
Average of 6 runs Standard Deviations Shown



Average of 6 runs Smoothed Data







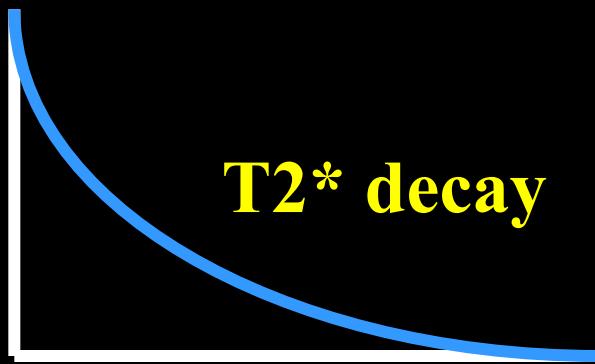
Variables to Optimize

- Information Content
- Sensitivity
- Acquisition Speed
- Resolution
- Image quality

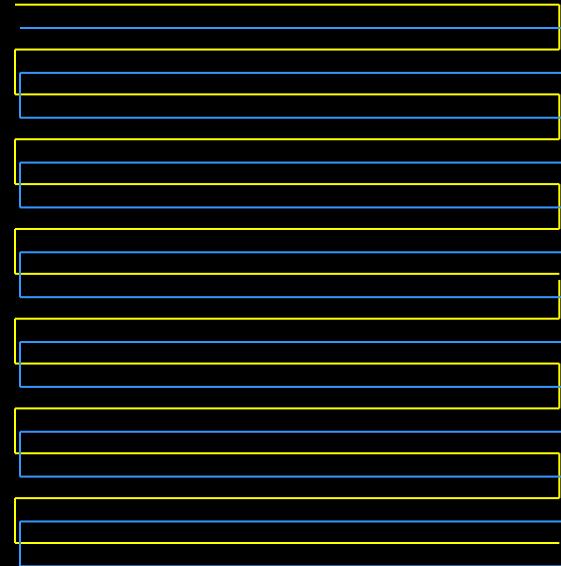
Multishot Imaging



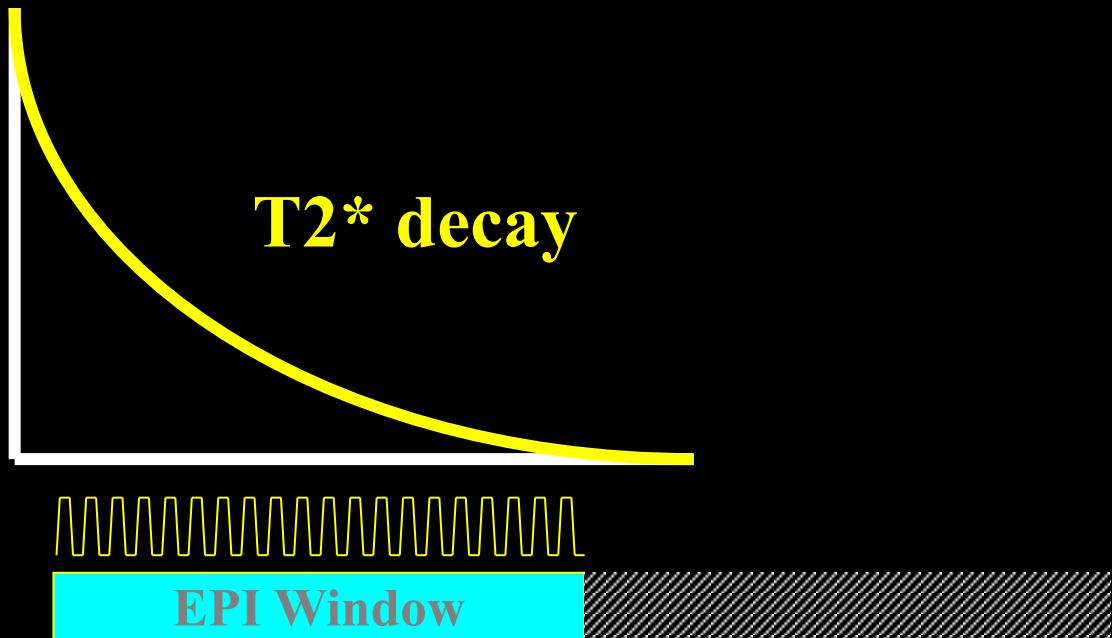
EPI Window 1



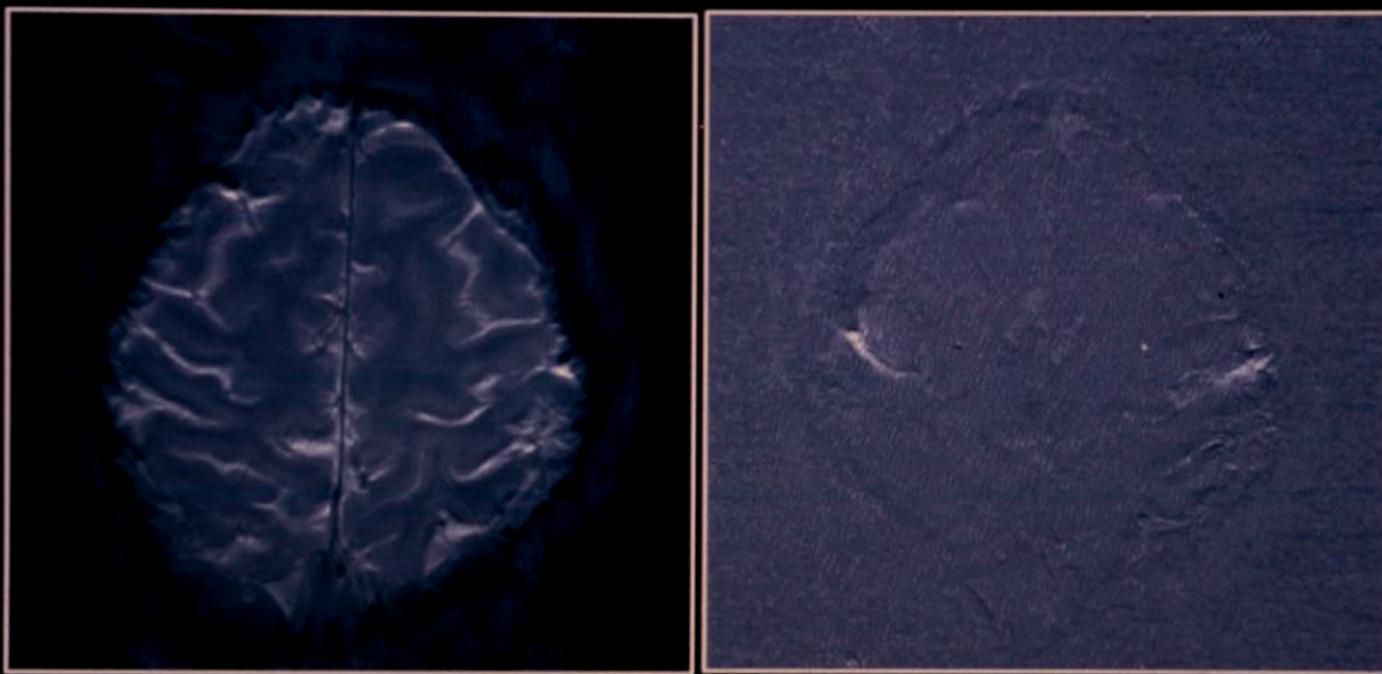
EPI Window 2



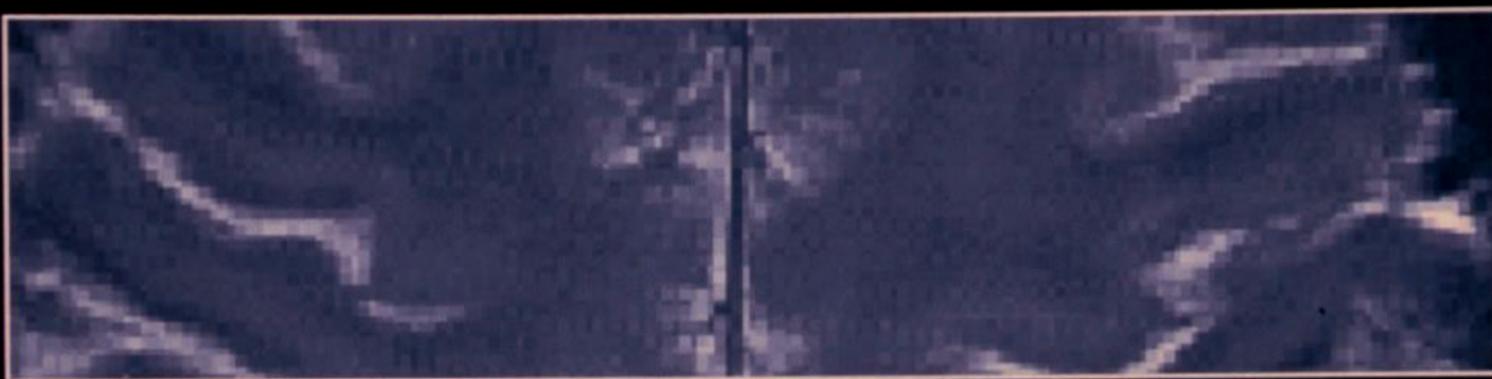
Partial k-space imaging



**Single - Shot EPI at 3T:
Half NEX, 256 x 256, 16 cm FOV**



**Single - Shot EPI at 3T:
Half NEX 256 x 256, 16 cm FOV**



Multi Shot EPI

Excitations

1

Matrix Size

64 x 64

2

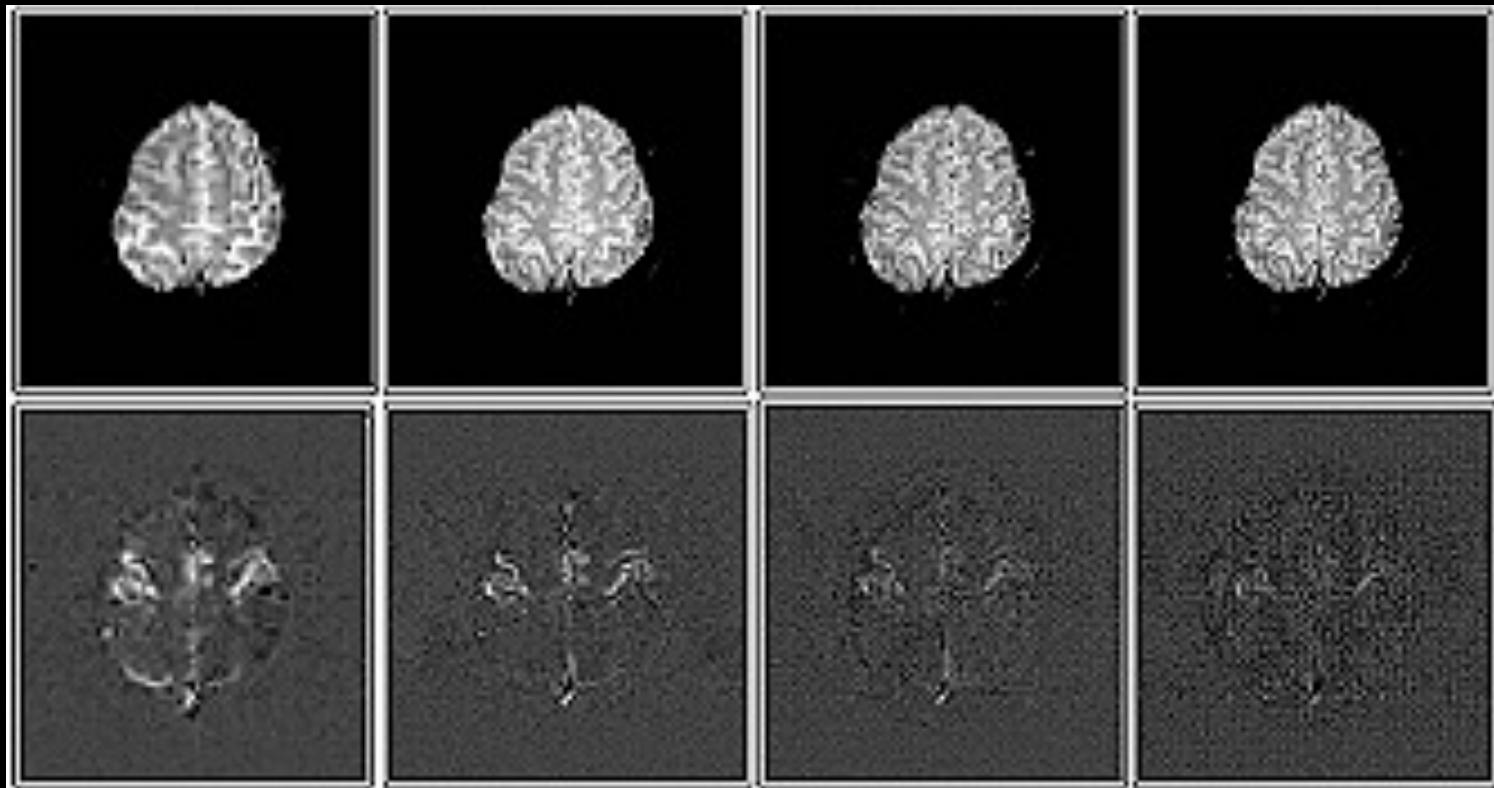
128 x 128

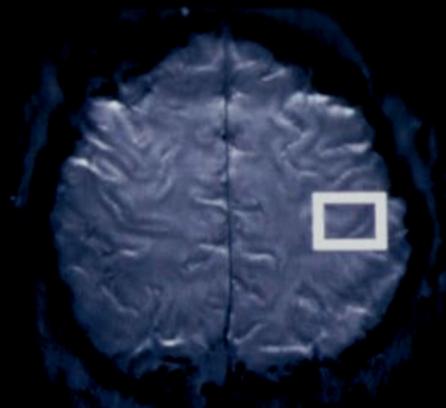
4

256 x 128

8

256





64 x 64

96 x 96

128 x 128

192 x 192

256 x 256

%



C/N



2.5 mm²

1.67 mm²

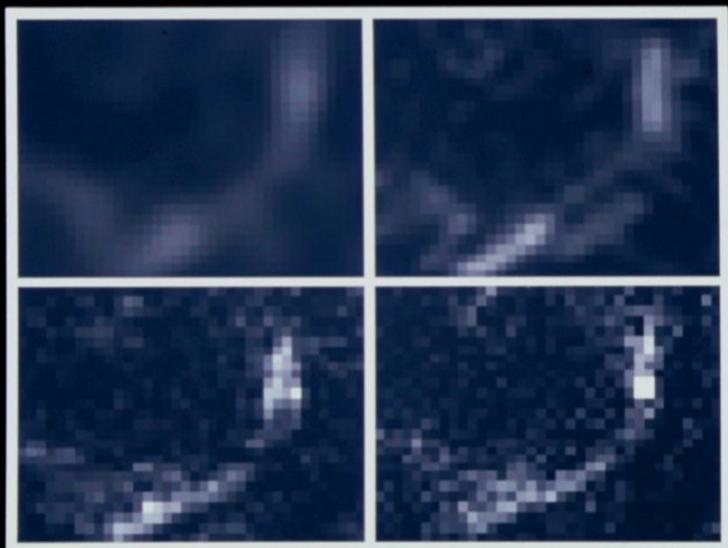
1.25 mm²

0.83 mm²

0.62 mm²

Fractional Signal Change

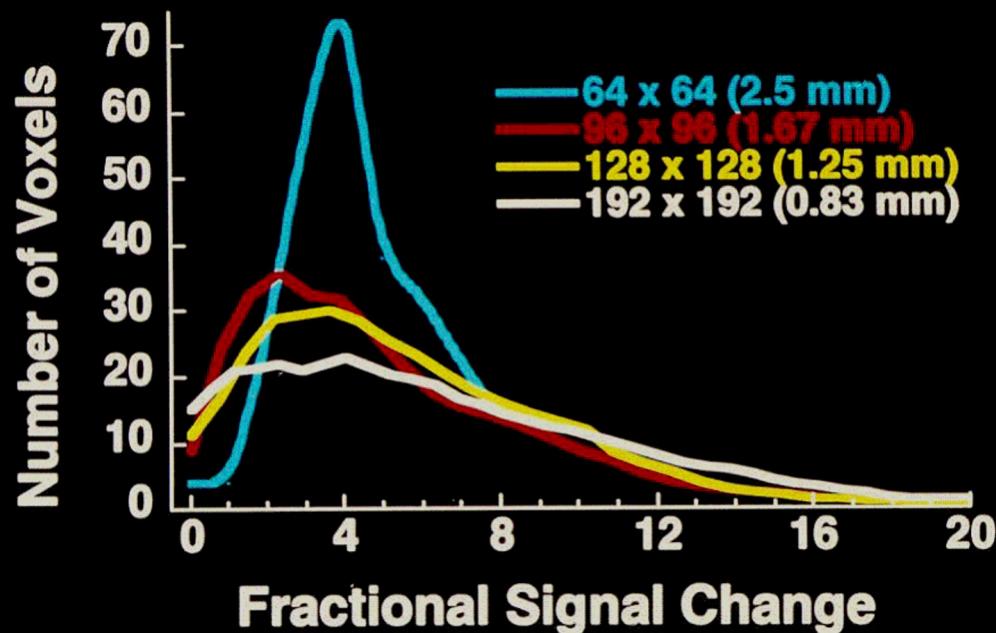
2.5 mm^2



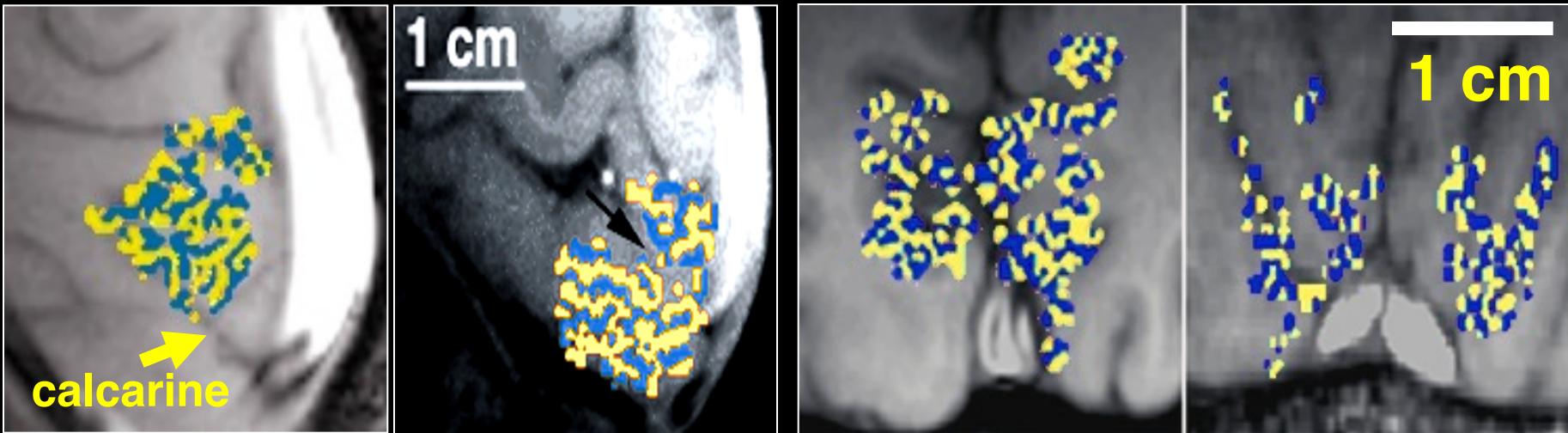
1.25 mm^2

0.83 mm^2

0.62 mm^2



ODC Maps using fMRI



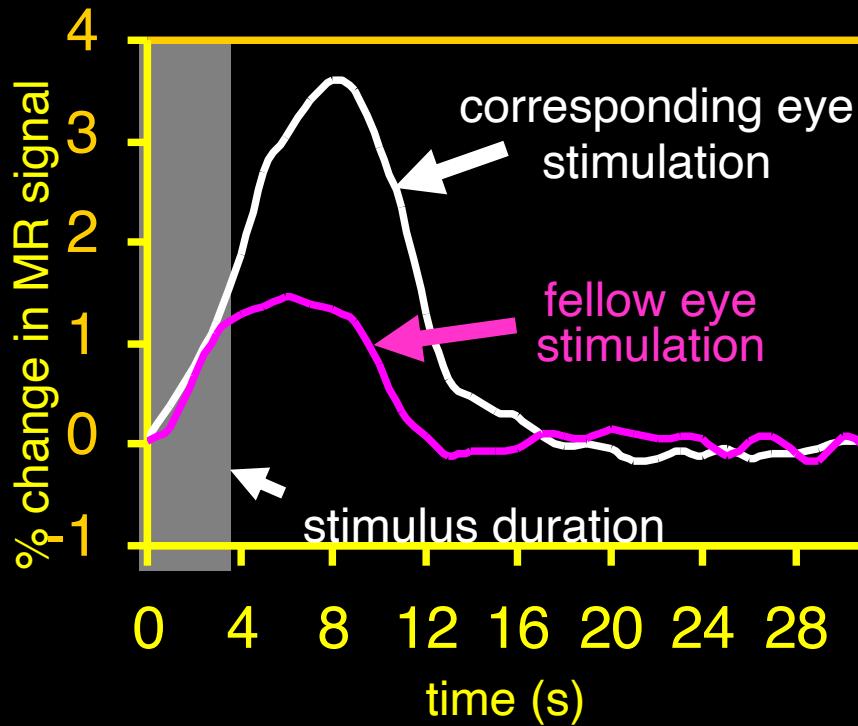
- Identical in size, orientation, and appearance to those obtained by optical imaging¹ and histology^{3,4}.

¹Malonek D, Grinvald A. *Science* 272, 551-4 (1996).

³Horton JC, Hocking DR. *J Neurosci* 16, 7228-39 (1996).

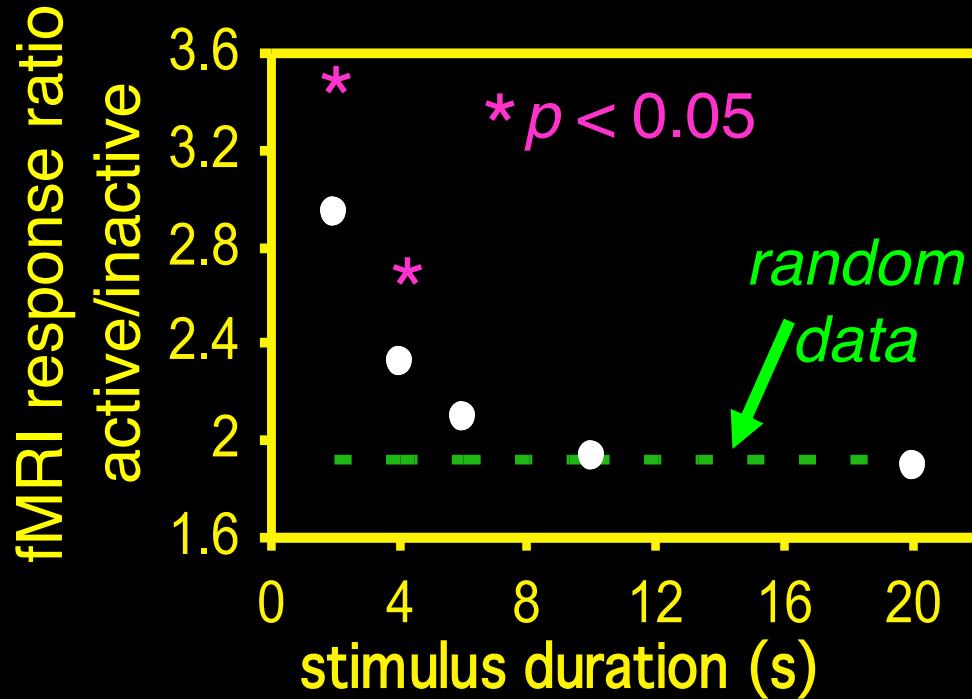
⁴Horton JC, et al. *Arch Ophthalmol* 108, 1025-31 (1990).

fMRI Timecourse within an ODC



- For a 4 second stimulus, the hyperoxic response does not saturate (i.e., does not reach a plateau).
- The ratio of the peak magnitudes of the fMRI responses is nearly 3:1.

Experiment 2: Stimulus Duration



- The saturation of the hyperoxic response does not permit reliable mapping of ODCs.
- ODC maps obtained using the hyperoxic phase of the BOLD fMRI signal *are* reliable when stimulus duration is 4 seconds or less.

Variables to Optimize

- Information Content
- Sensitivity
- Speed
- Resolution
- Image quality

Image Quality

- Minimizing warping
 - Shimming
 - Reduced readout window duration
- Minimizing dropout
 - Shimming
 - Reduced TE
 - Adjust slice orientation
 - Increase resolution

Neuronal Activation Input Strategies

1. Block Design

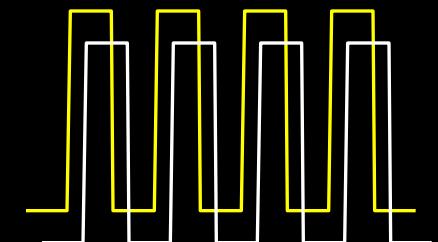
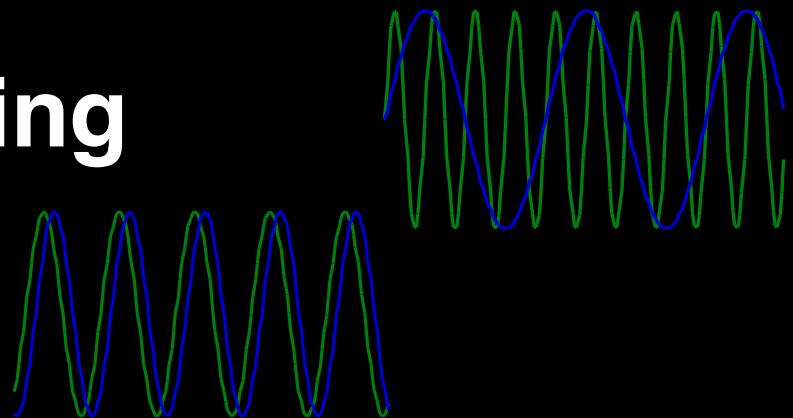
2. Frequency Encoding

3. Phase Encoding

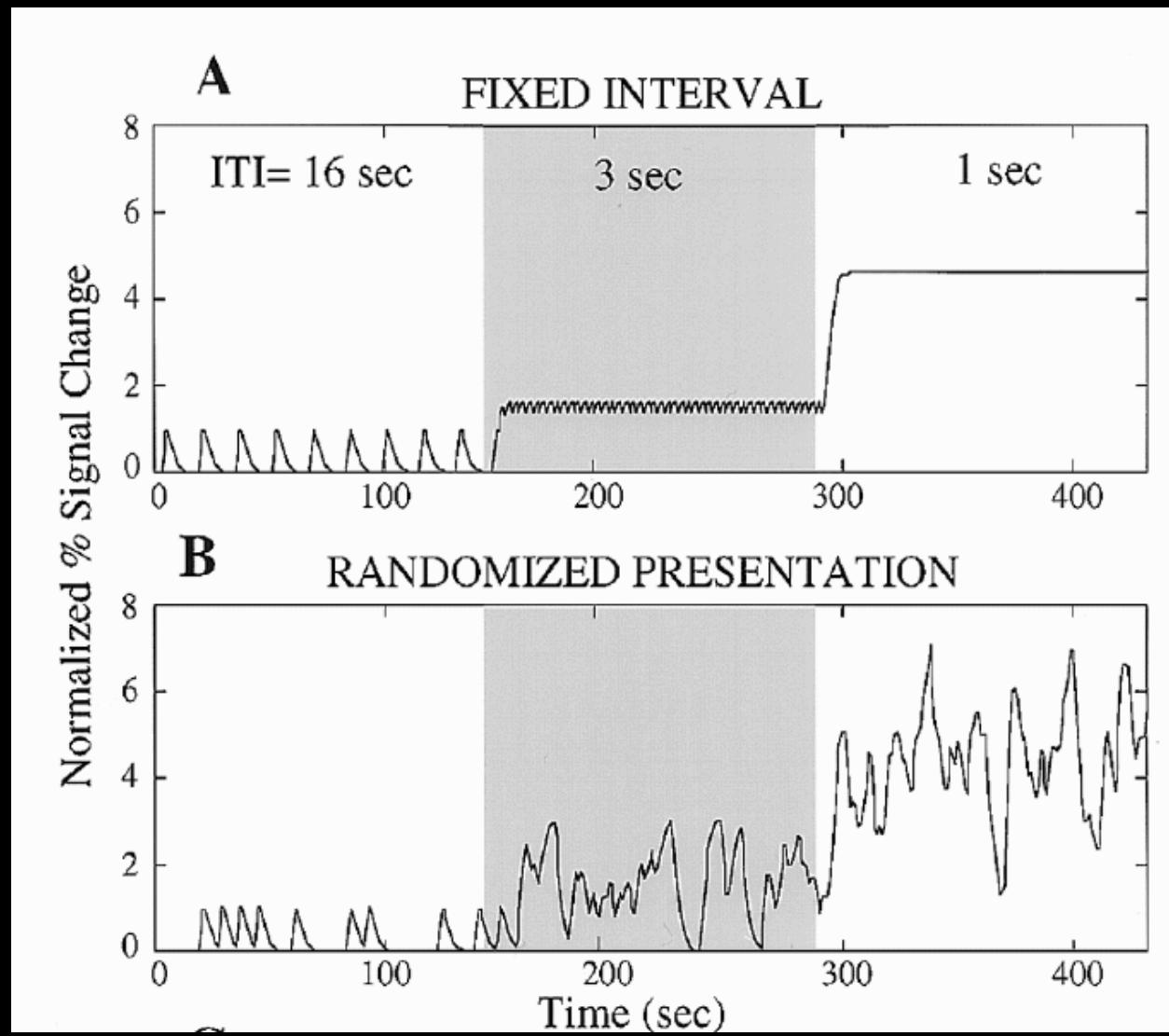
4. Event Related

5. Orthogonal Block Design

6. Free behavior Design.

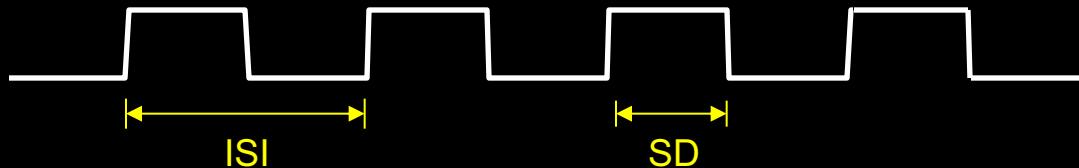


M.A. Burock et al. *NeuroReport*, 9, 3735-9 (1998)

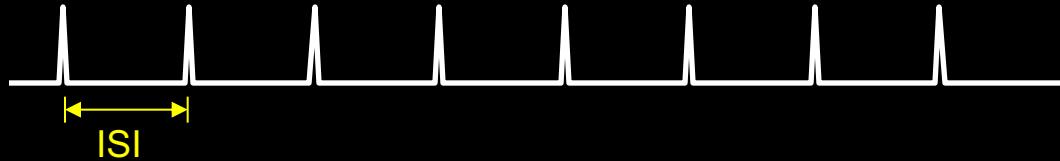


Definitions

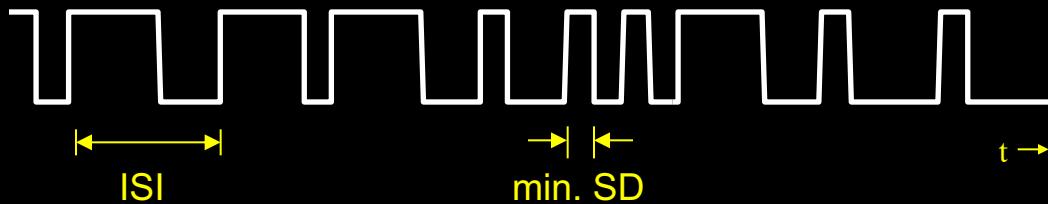
Blocked Trial



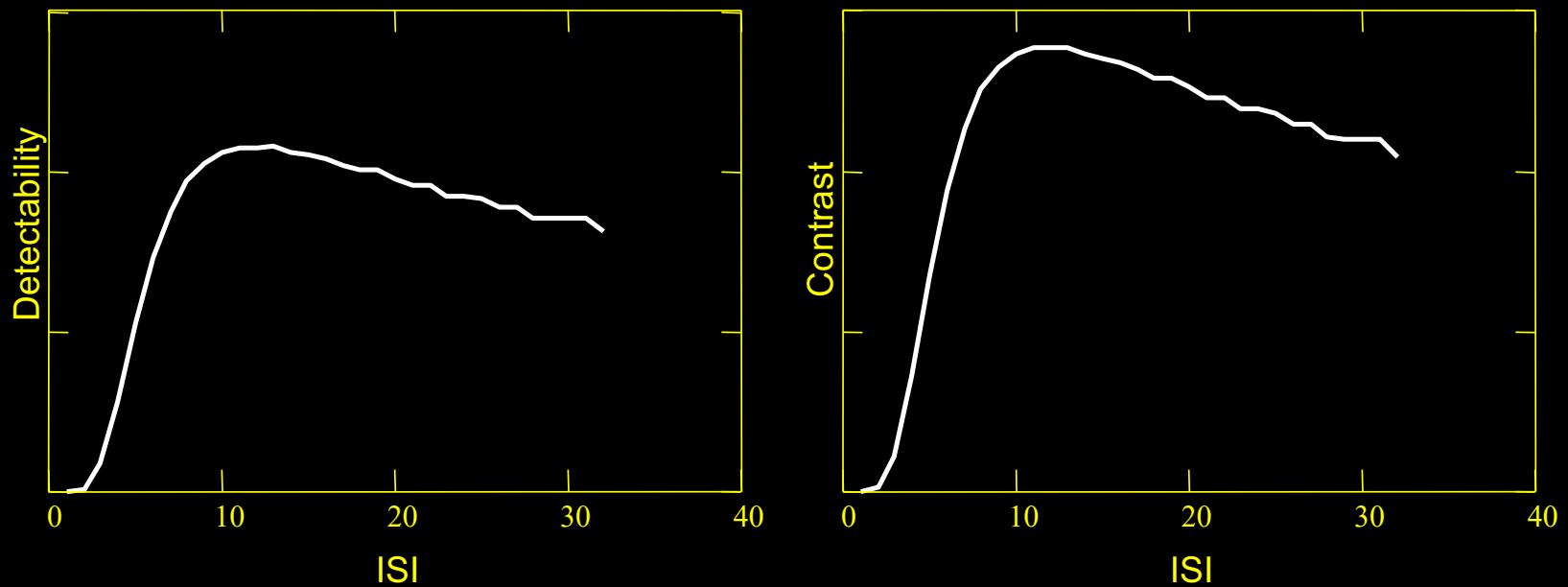
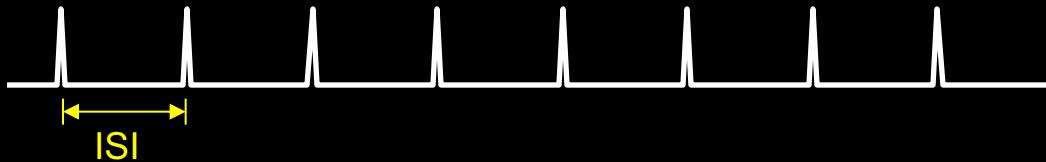
Event-Related
Constant ISI



Event-Related
Variable ISI

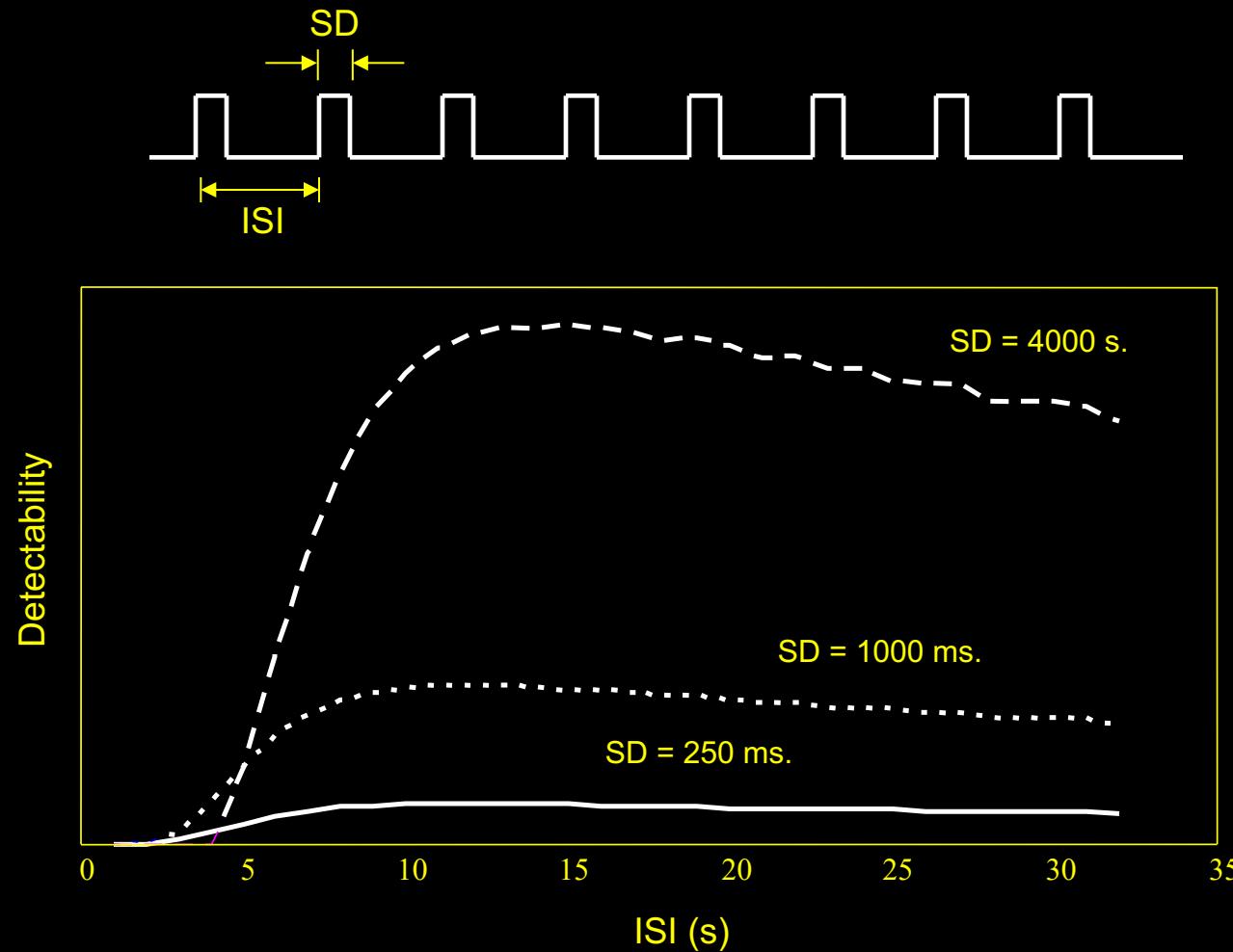


Detection – constant ISI



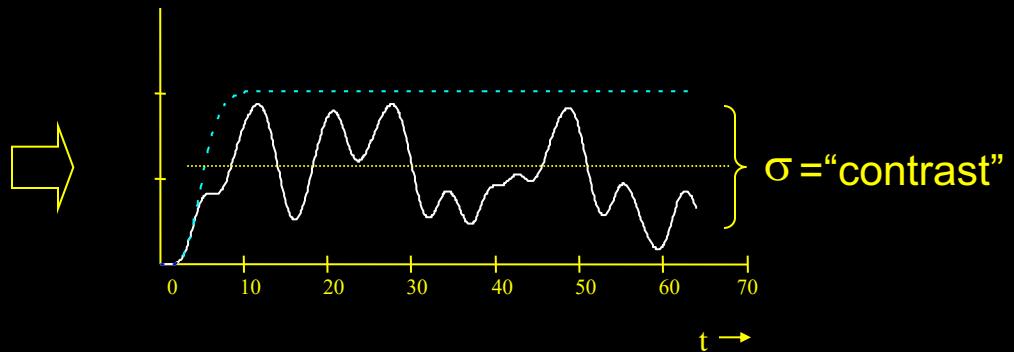
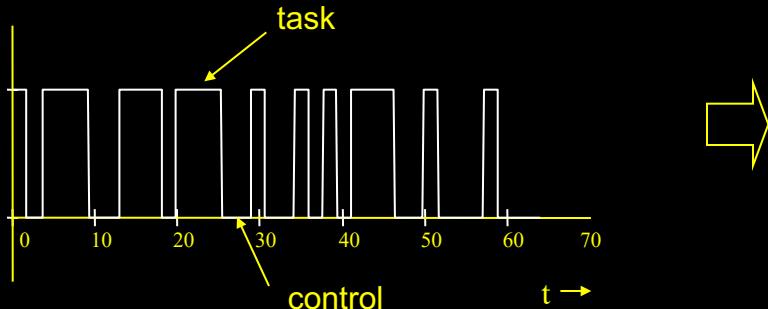
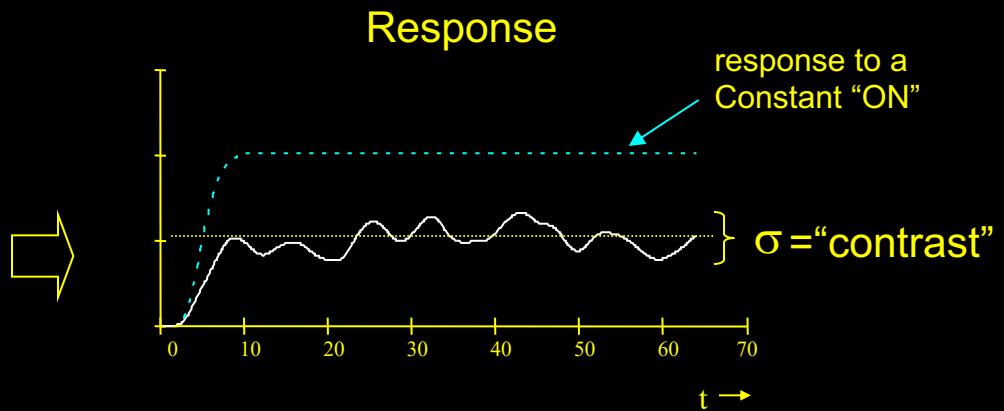
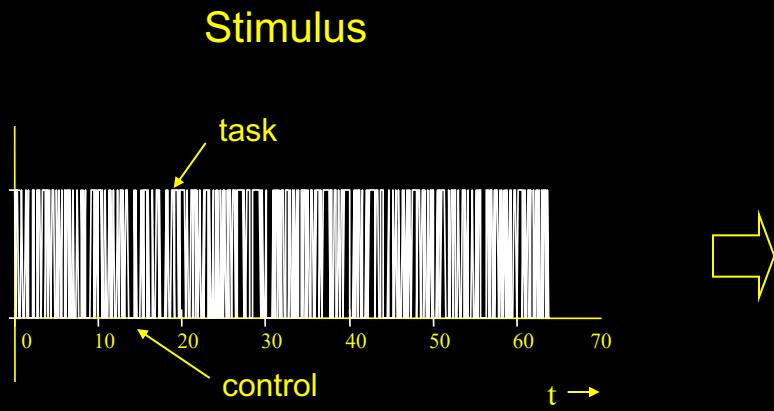
Optimal detection when there is no overlap

Detection vs. ISI – different SD

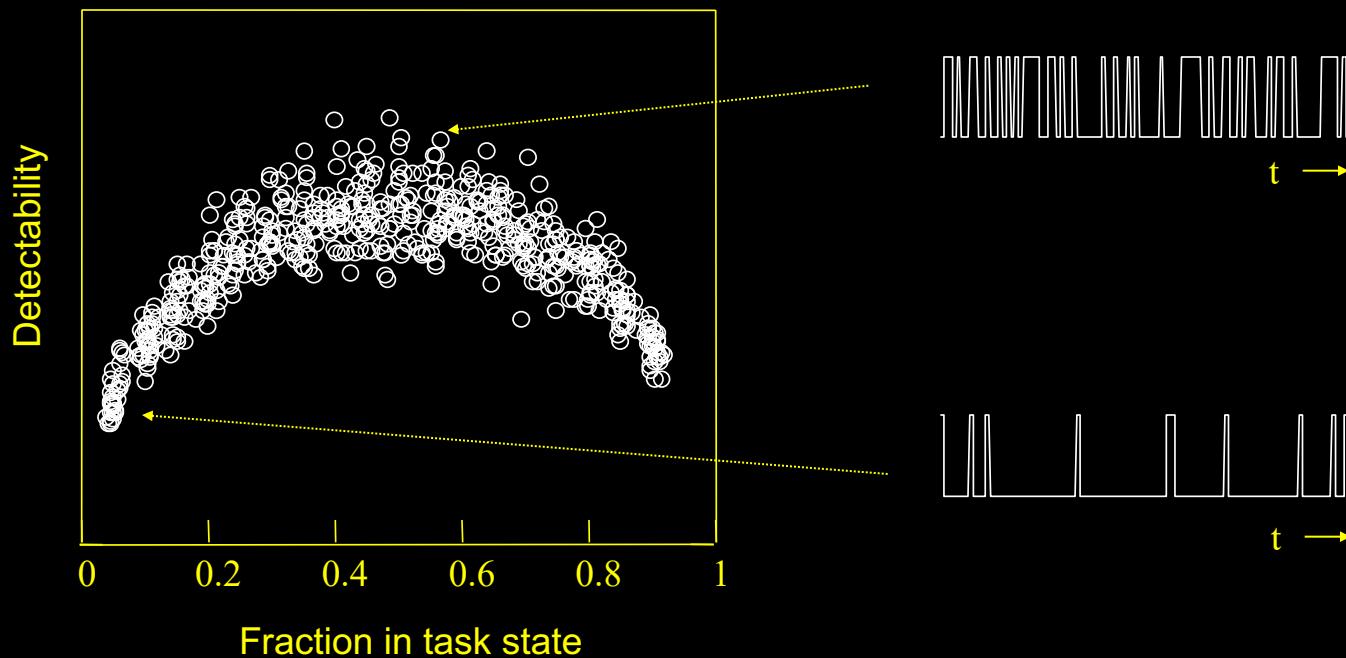


Optimal detection when there is no overlap

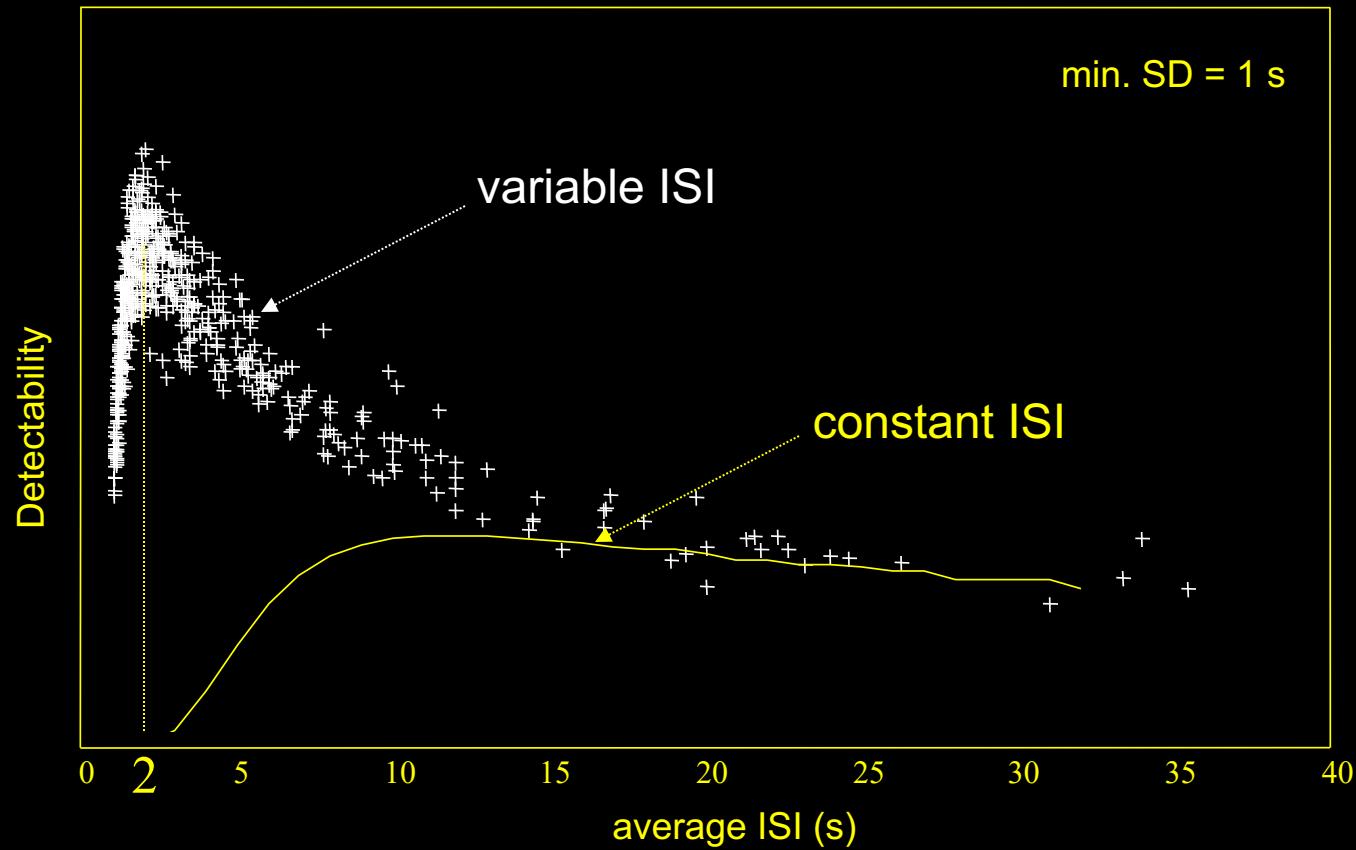
Detection: Contrast



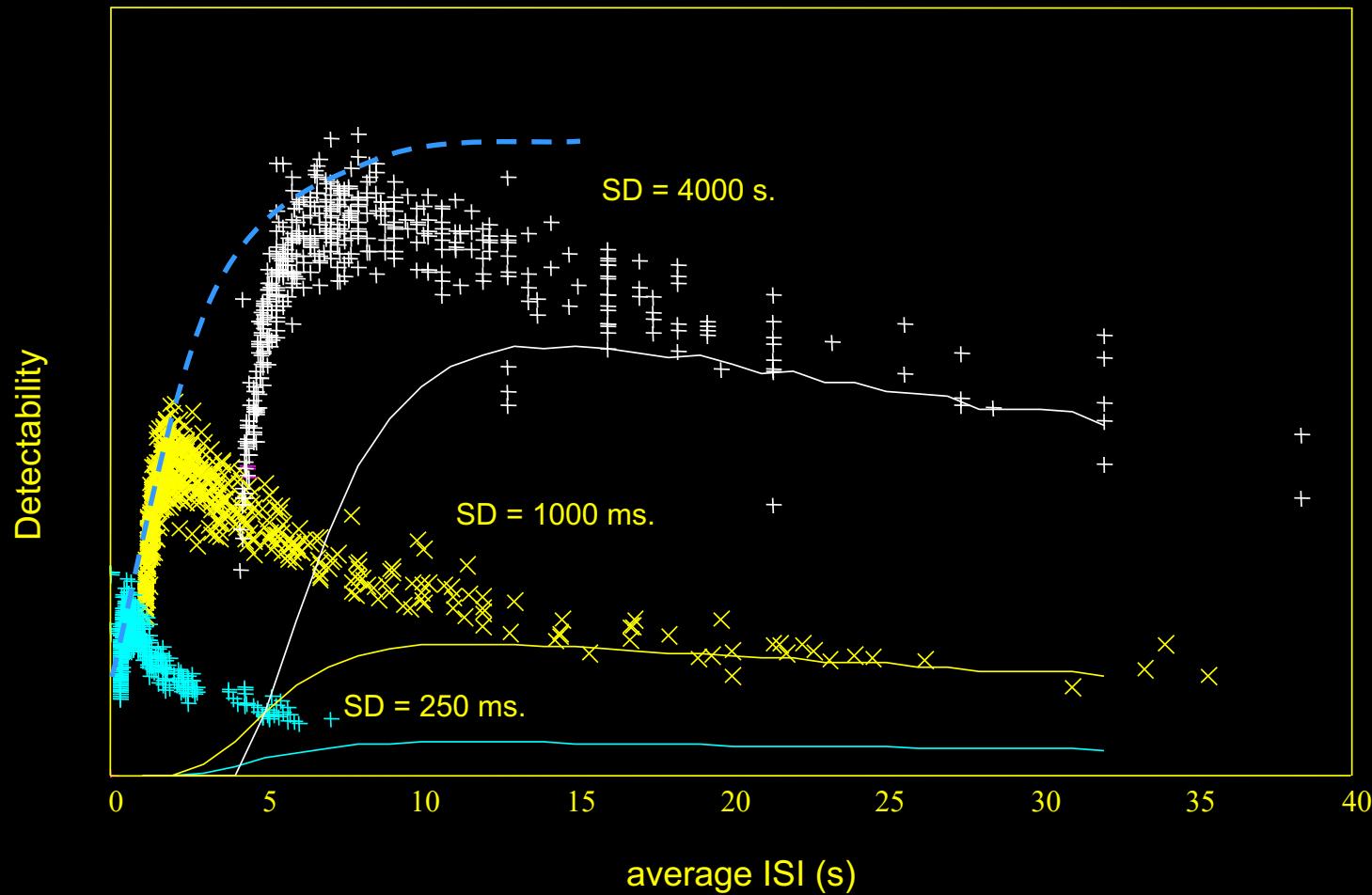
Detection vs. % “on” – variable ISI



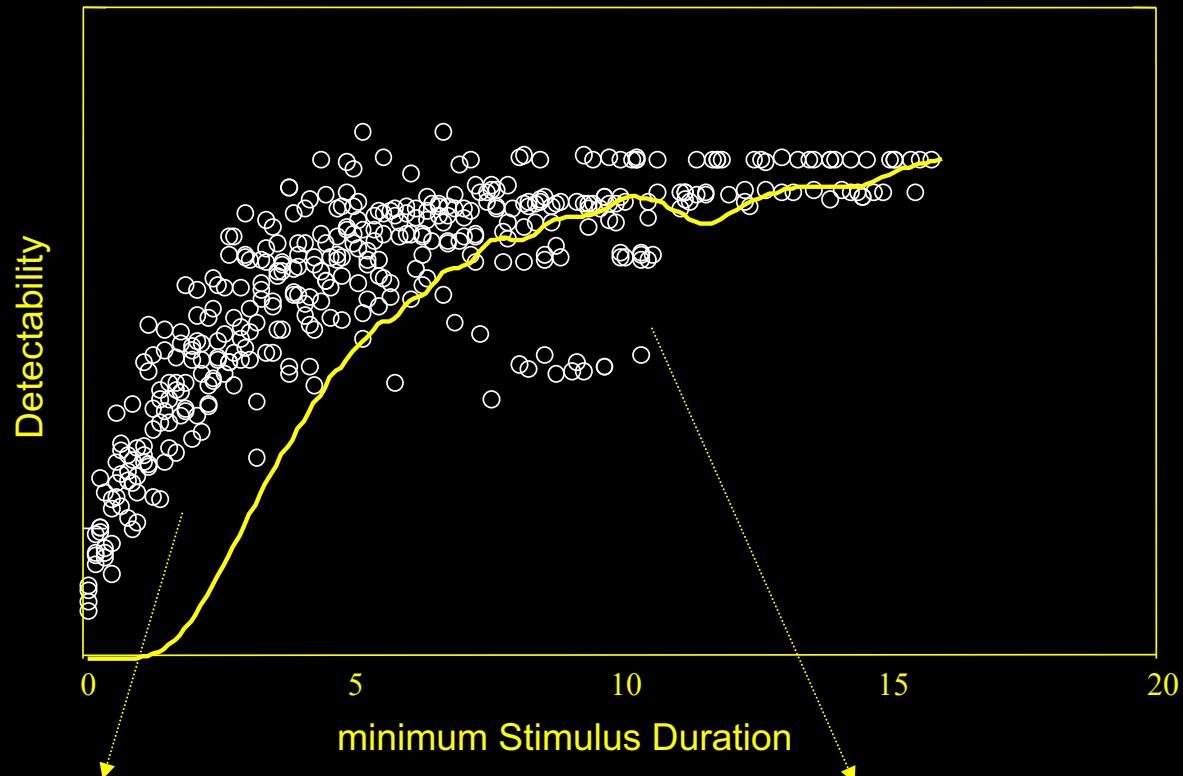
Detection vs. Average ISI



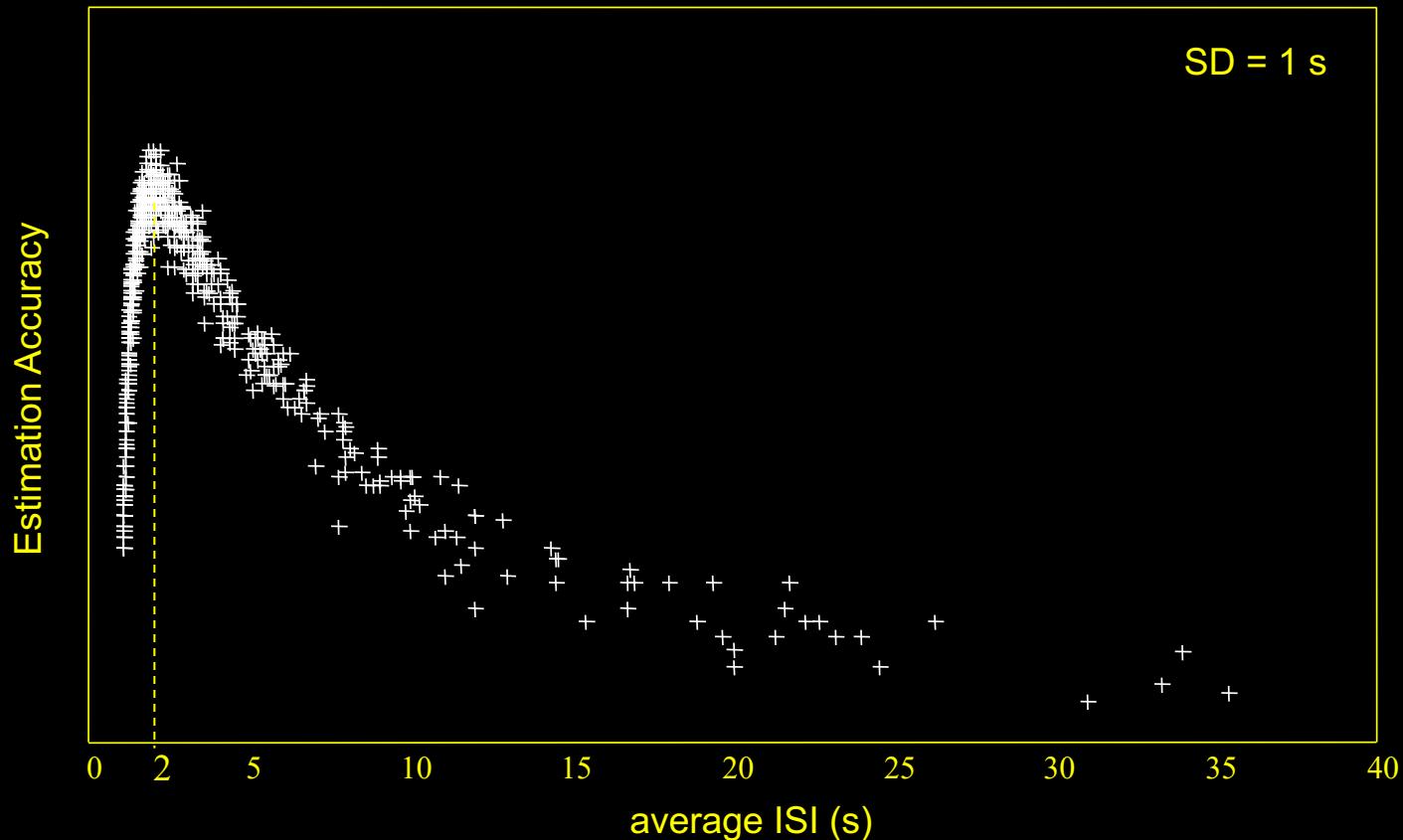
Detection vs. average ISI



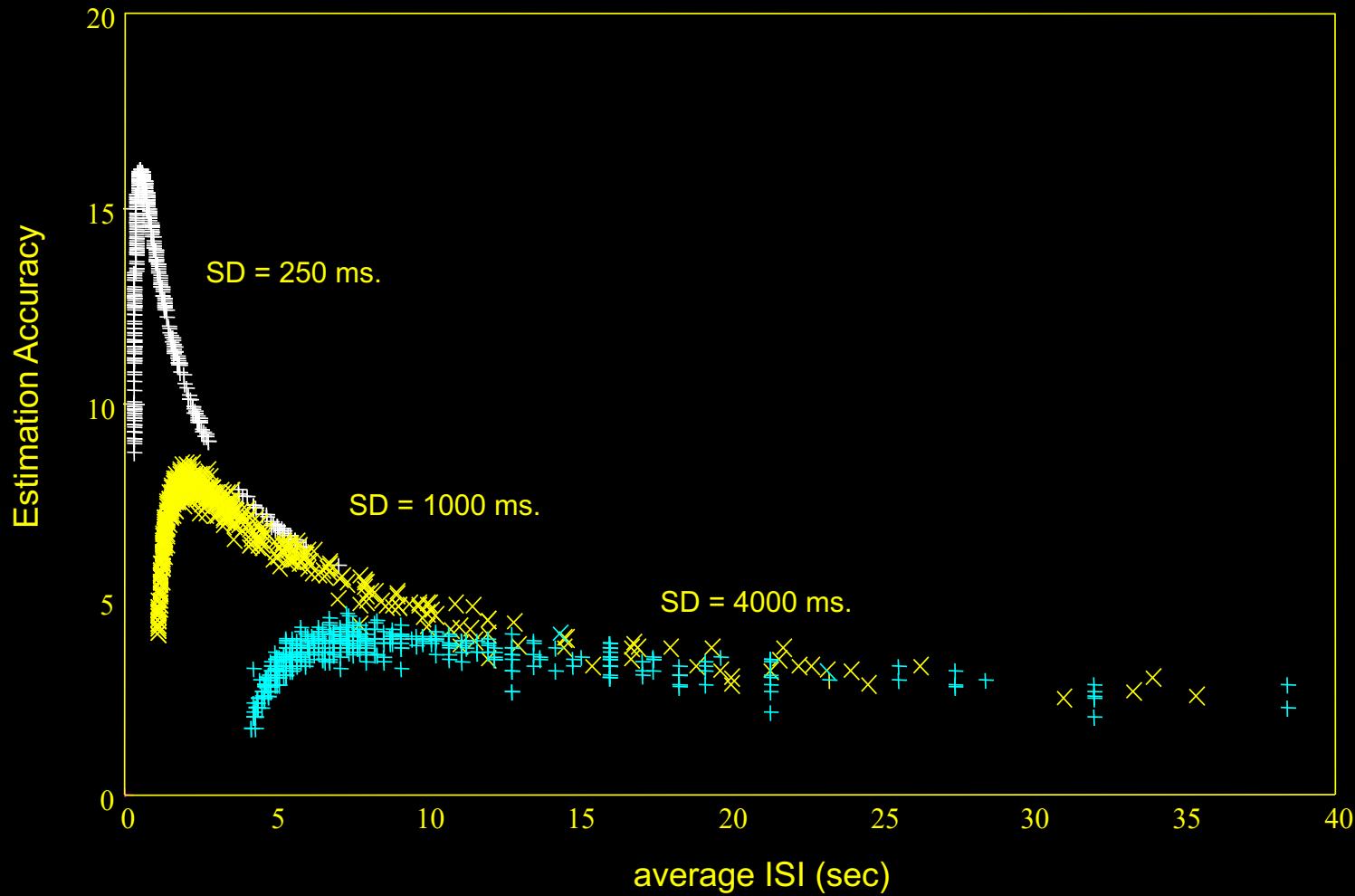
Detection – 50% “on”



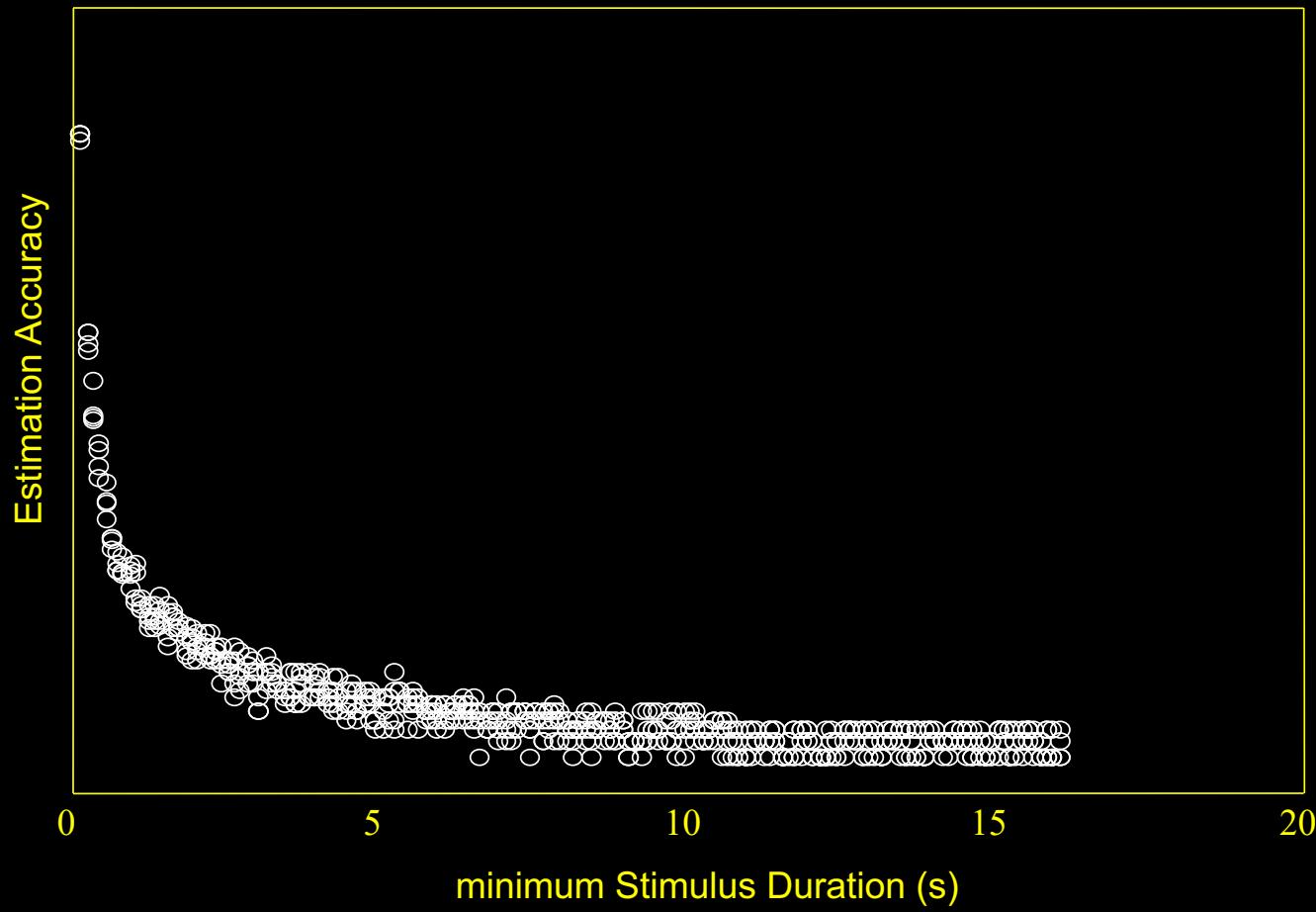
Estimation accuracy vs. average ISI



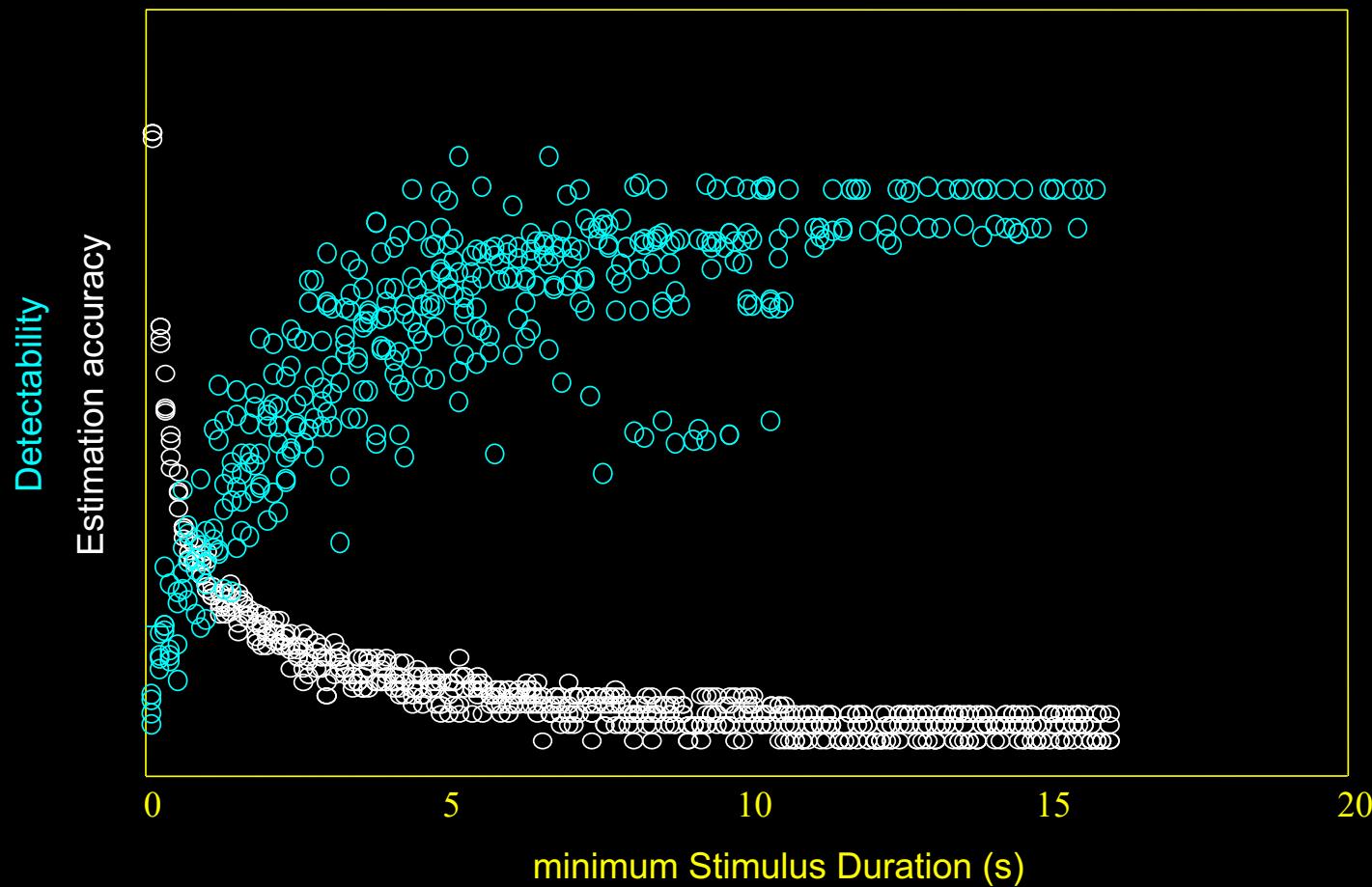
Estimation accuracy vs. average ISI



Estimation accuracy – 50% “on”



Detection and Estimation



Acknowledgements

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&...

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Jerzy Bodurka

Post Docs:

Rasmus Birn

Patrick Bellgowan

Ziad Saad

Clinical Fellow:

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Natalia Petridou

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Hannah Chang

Courtney Kemps



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