

How Much Neuronal Information Advancing fMRI Utility Can We Extract With fMRI?

Peter A. Bandettini, Ph.D

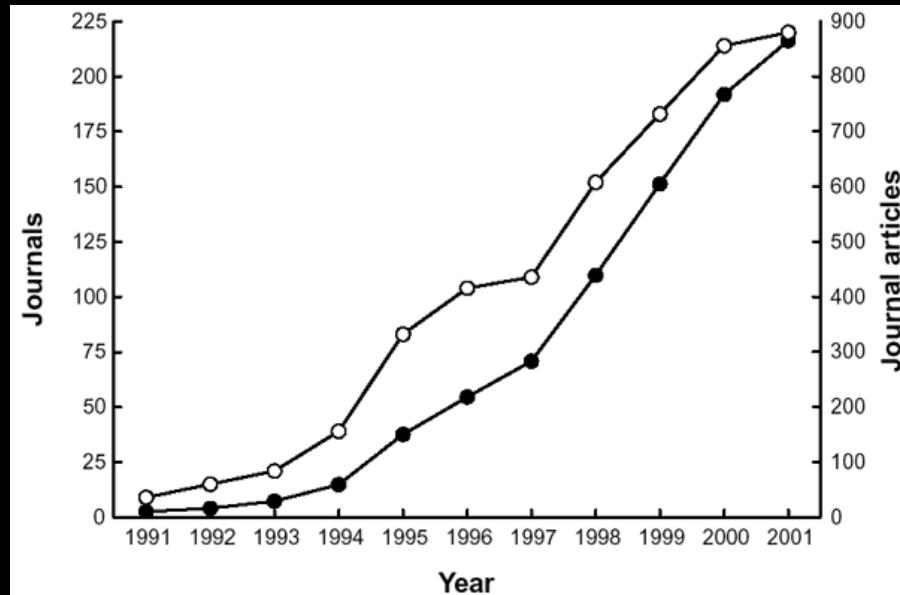
bandettini@nih.gov

Unit on Functional Imaging Methods
&
Functional MRI Facility

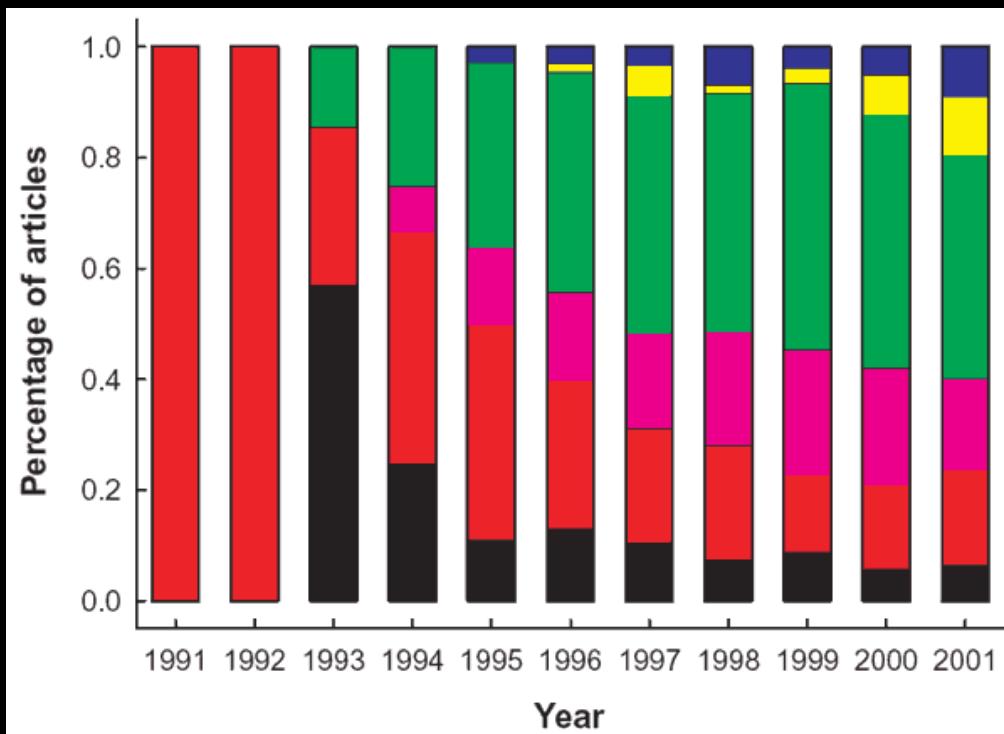
Laboratory of Brain and Cognition
National Institute of Mental Health



J. Illes, M. P. Kirschchen,
J. D. E. Gabrielli,
Nature Neuroscience,
6 (3)m p.205



Motor (black)
Primary Sensory (red)
Integrative Sensory (violet)
Basic Cognition (green)
High-Order Cognition (yellow)
Emotion (blue)



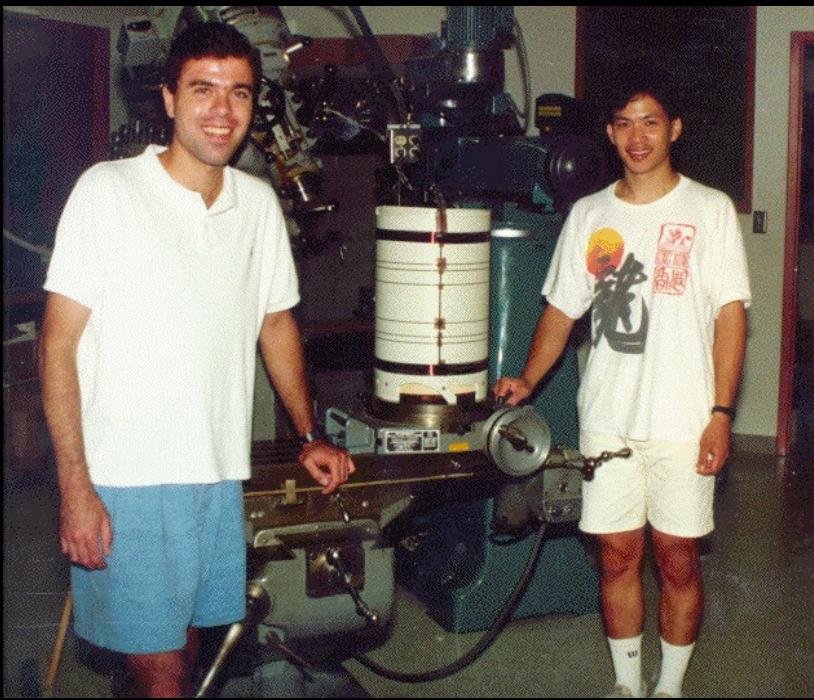
Most fMRI studies since 1992:

Minimum necessary:

- Whole Brain EPI
- Field strength of 1.5T or greater
- Basic stimulus delivery and feedback
- Software for image transfer, analysis, and display

Typical advanced features:

- Higher resolution whole brain EPI, spiral, or multi-shot
- Field strength of 3T to 7T
- Quadrature and Surface coils (single, multiple)
- Susceptibility correction
- ASL (perfusion imaging)
- Multiple subject interface devices, including EEG, SCR, eye position.
- Multi-subject analysis, more rigorous statistics, more sophisticated display methods, exploratory analysis



1991-1992



1992-1999



Technology

MRI	EPI	1.5T,3T, 4T	EPI on Clin. Syst.		Diff. tensor	Mg ⁺	7T	>8 channels
		Local Human Head Gradient Coils	Nav. pulses	Real time fMRI	Venography		SENSE	"vaso"
		ASL	Spiral EPI	Quant. ASL	Z-shim			
		BOLD	Multi-shot fMRI	Dynamic IV volume	Simultaneous ASL and BOLD		Baseline Susceptibility	
							Current Imaging?	

Methodology

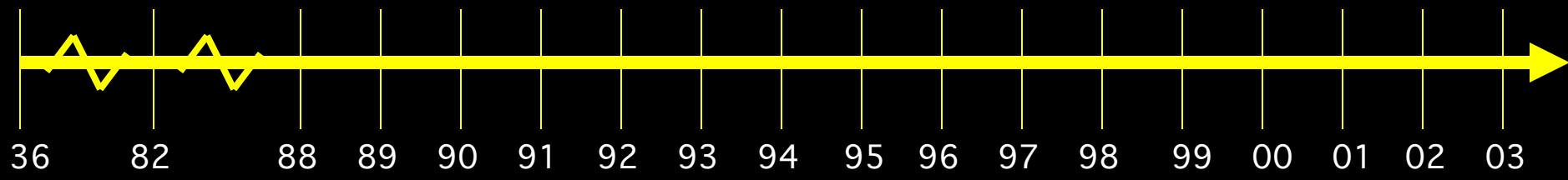
IVIM	Baseline Volume	Correlation Analysis		CO ₂ Calibration				
		Motion Correction				Latency and Width Mod		
		Parametric Design		Multi-Modal Mapping				
		Surface Mapping						
		Phase Mapping		ICA	Free-behavior Designs			
		Linear Regression		Mental Chronometry		Multi-variate Mapping		
		Event-related		Deconvolution	Fuzzy Clustering			

Interpretation

Blood T2	BOLD models	PET correlation						
	B ₀ dep.	IV vs EV	ASL vs. BOLD			Layer spec. latency		
		Pre-undershoot	PSF of BOLD					
	TE dep	Resolution Dep.		Extended Stim.			Excite and Inhibit	
		Post-undershoot						
	SE vs. GE	CO ₂ effect		Linearity		Metab. Correlation		
	NIRS Correlation		Fluctuations	Optical Im. Correlation				
	Veins	Inflow	Balloon Model			Electrophys. correlation		

Applications

Volume - Stroke	Complex motor							
	Language	Imagery	Memory			Emotion	Epilepsy	
				Motor learning	Children	Tumor vasc.	Drug effects	
	BOLD -V1, M1, A1	Presurgical	Attention		Ocular Dominance		Mirror neurons	
	V1, V2..mapping		Priming/Learning		Clinical Populations			
	△ Volume-V1		Plasticity	Face recognition		Performance prediction		



Technology

Methodology

Engineering

Physics

Computer
Science

Statistics

Cognitive
Science

Neuroscience

Physiology

Medicine

Interpretation

Applications

What are the biggest unknowns/challenges?

1. Technology
2. Methodology
3. Interpretation

What are the biggest unknowns/challenges?

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Technology

- Field strength
- Signal to noise
- Resolution
- Shimming

Field strength

Plusses

- SNR proportional to B_0
- Contrast proportional to B_0

Minuses

- Susceptibility effects increase
- RF penetration problems
- SAR problems
- Fluctuations increase

Bottom Line

- SNR buys resolution when technology catches up
- Fluctuations may be increasingly interesting

Signal to noise

Methods to increase

- Increase B_0
- Smaller RF coils (arrays)
- Reduce noise

Issue:

- Temporal SNR is most important

More SNR...More “signal” is there...

The spatial extent of the BOLD response

Ziad S. Saad,^{a,b,*} Kristina M. Ropella,^b Edgar A. DeYoe,^c and Peter A. Bandettini^a

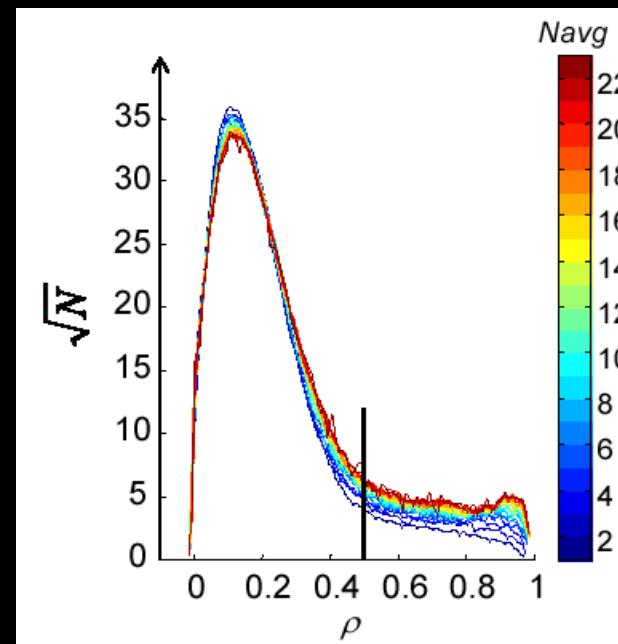
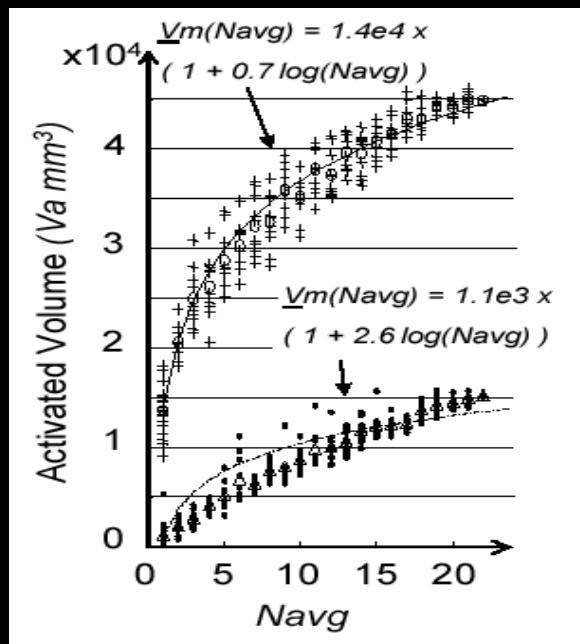
^a Laboratory of Brain and Cognition, National Institute of Mental Health, NIH, Bethesda, MD 20892-1148, USA

^b Department of Biomedical Engineering Marquette University, Milwaukee, WI 53233, USA

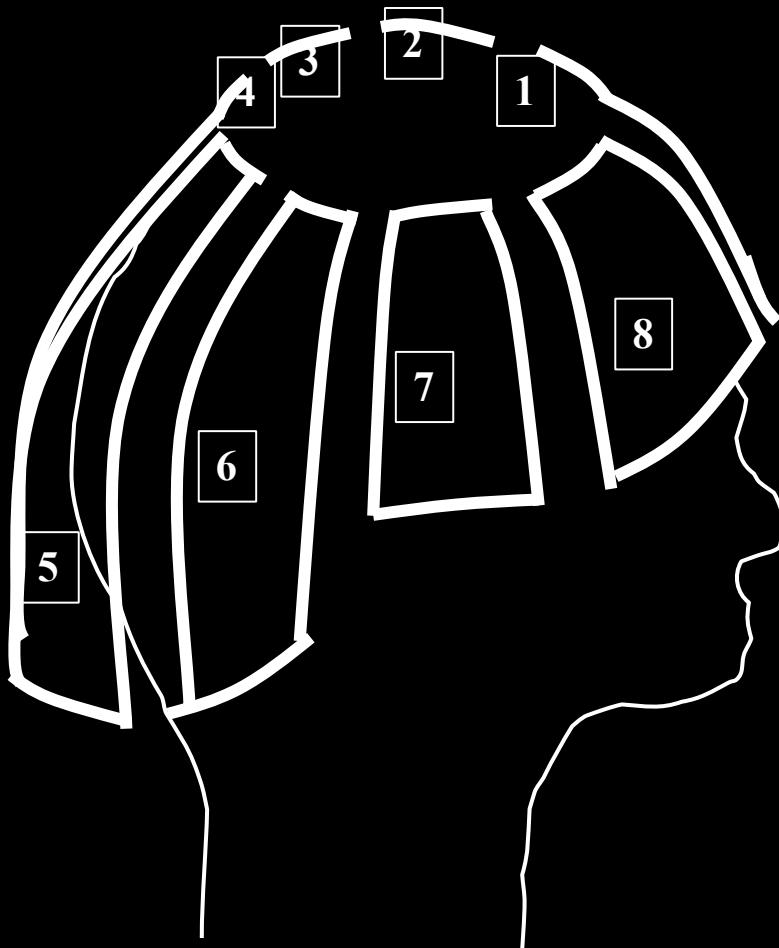
^c Department of Cell Biology, Neurobiology and Anatomy, Medical College of Wisconsin, Milwaukee, WI 53226, USA

Received 16 August 2002; revised 29 October 2002; accepted 21 November 2002

NeuroImage



General concept



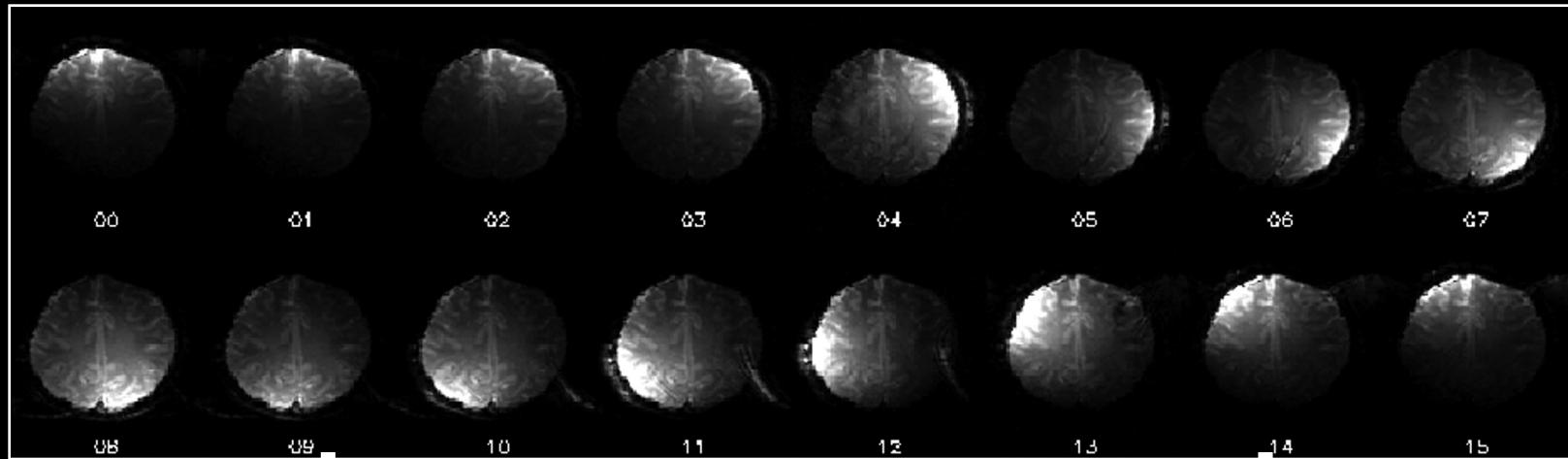
MRI Reception Hardware – 16 channels



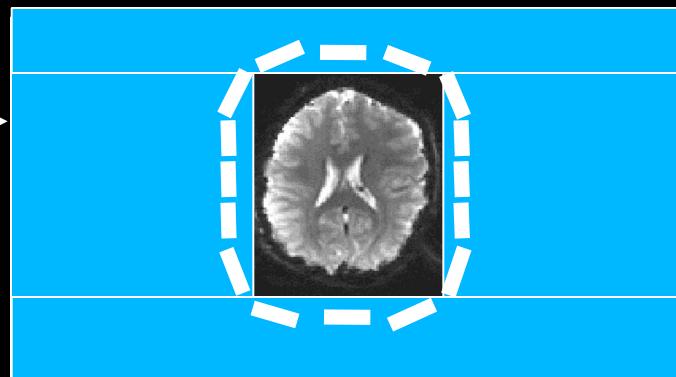
Built by Nova Medical Inc.

de Zwart et al. MRM 51:22 (2004).

Individual coil images

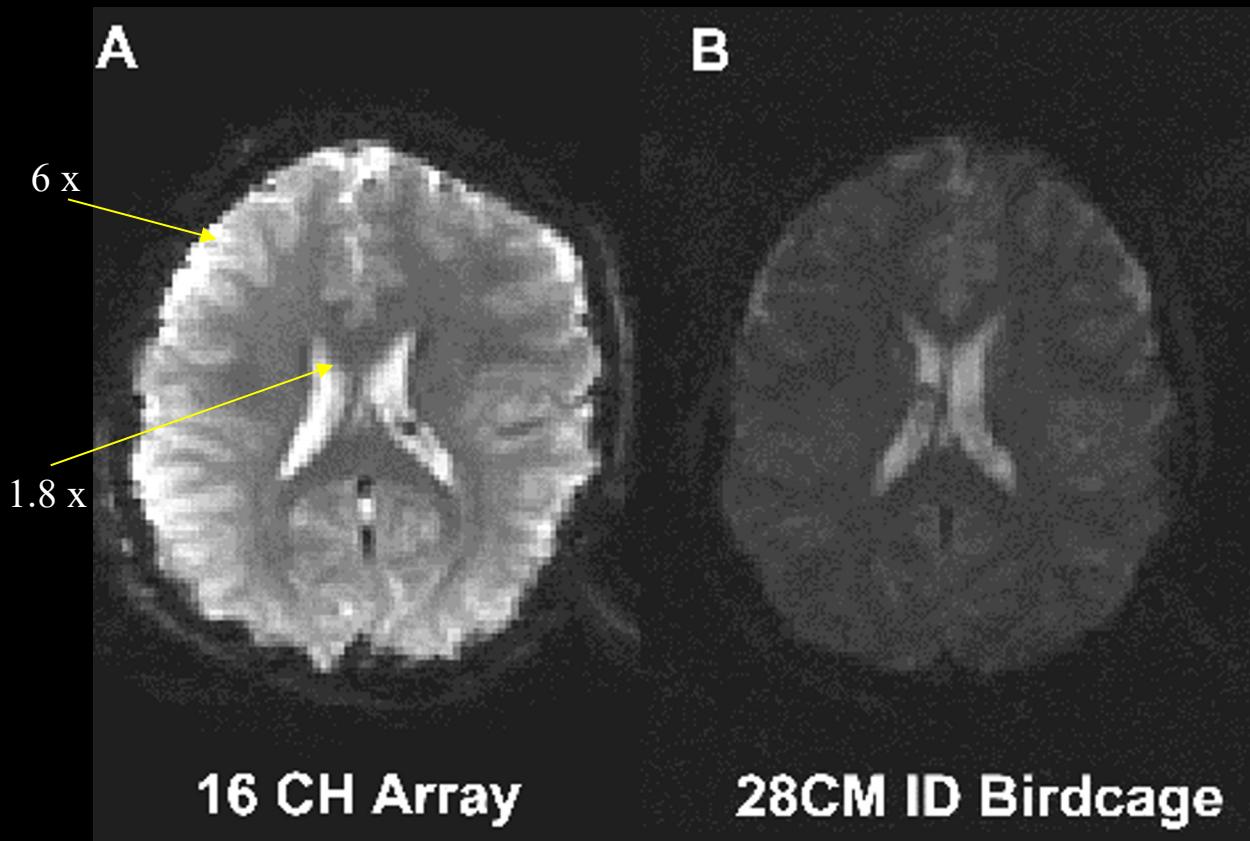


Single combined image



Experimental Data

SNR comparison



Both images are in the same scale.
Relative intensity corresponds to SNR.

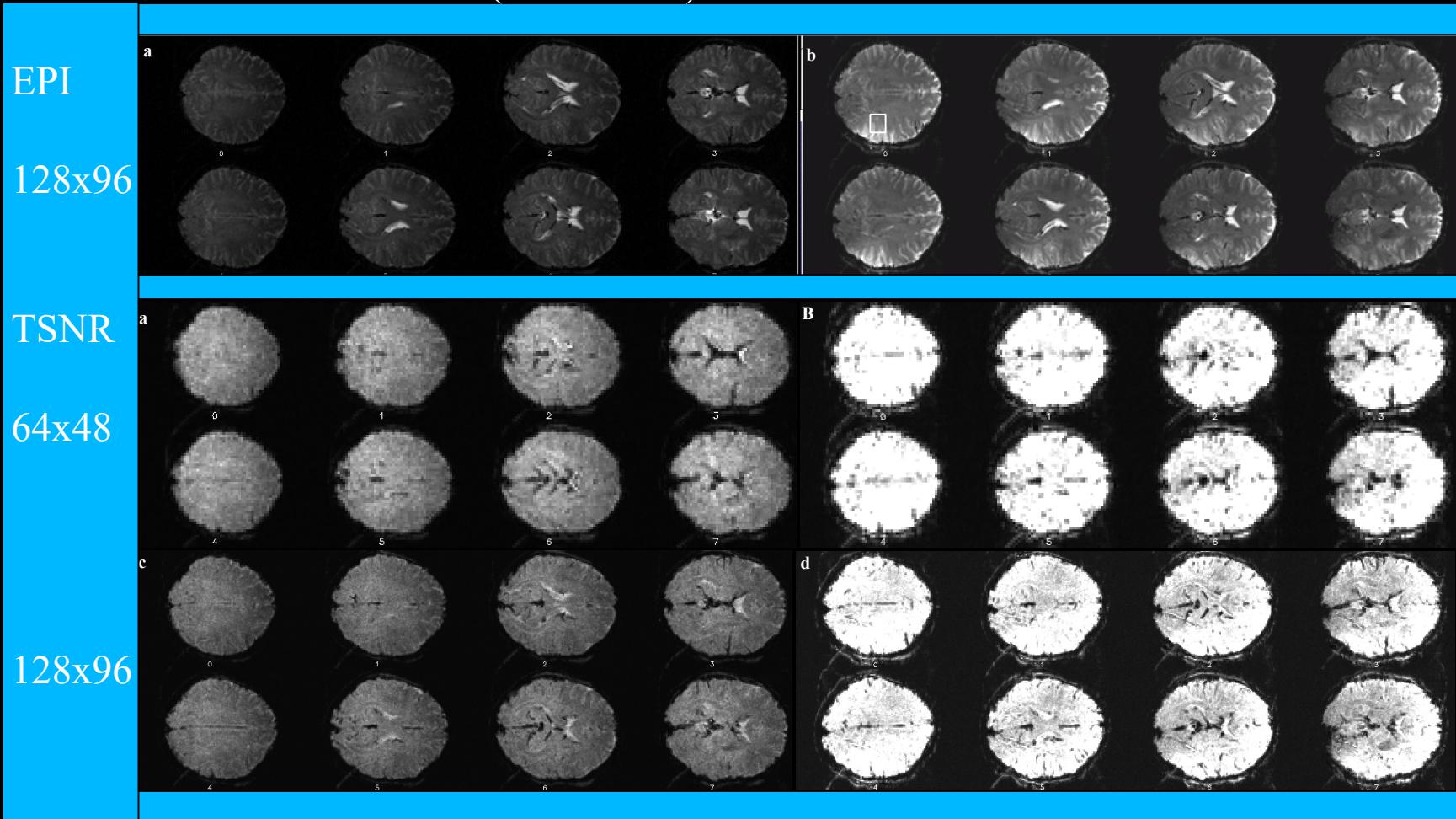
3-fold SNR improvements

Experimental Data

TSNR comparison

1 channel (MAI coil)

16 channel

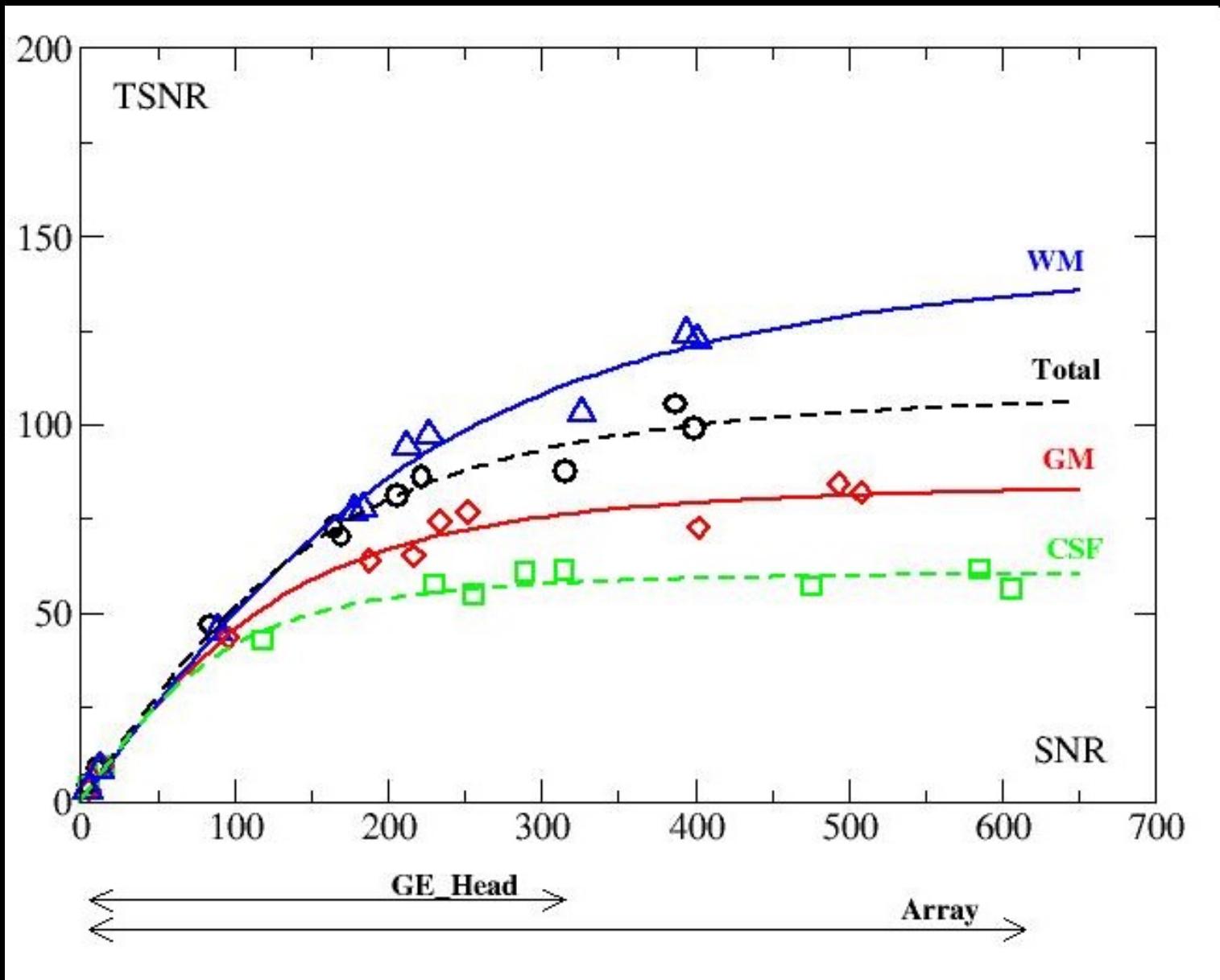


$\text{TSNR}_{16}/\text{TSNR}_1 :$

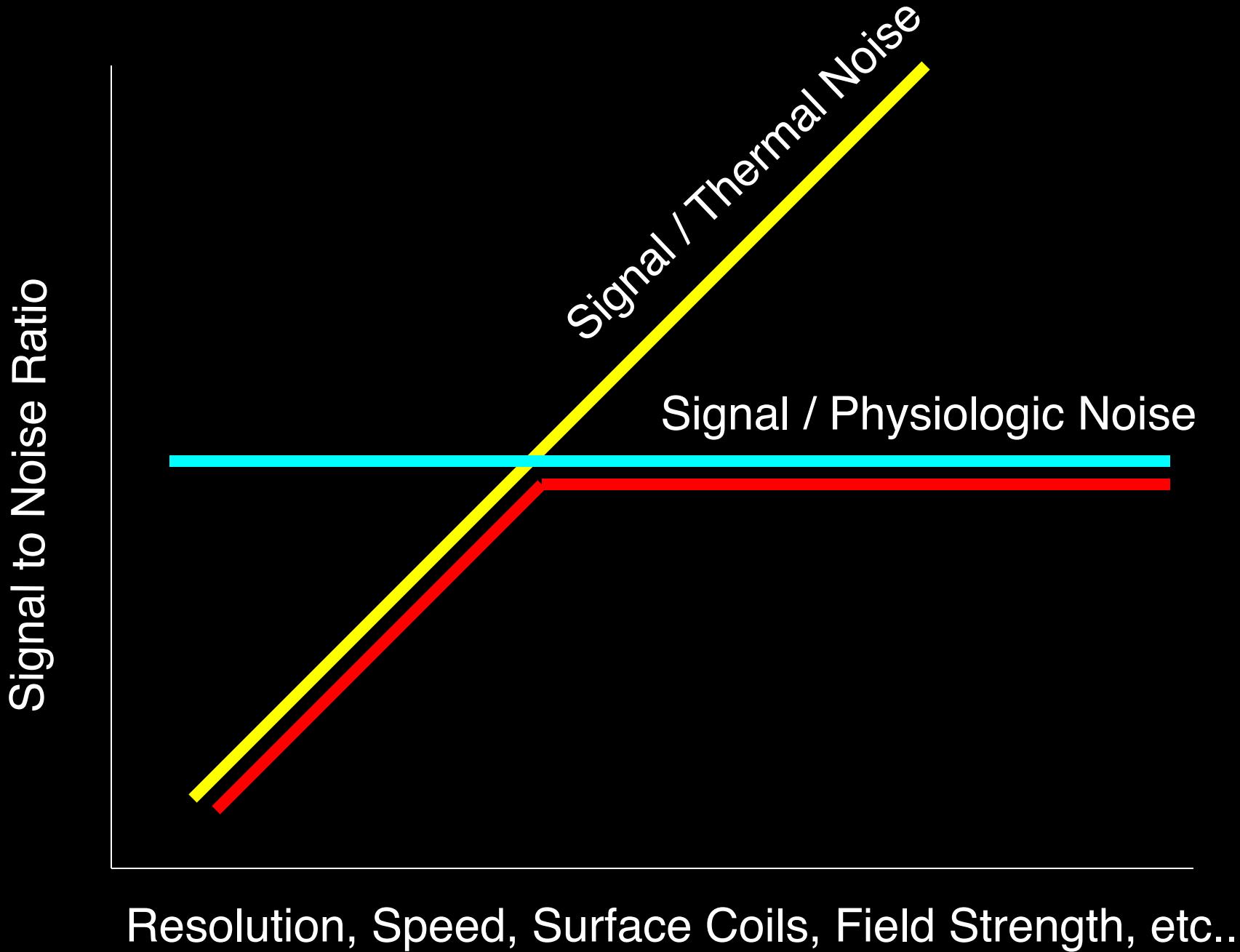
ROI: $64 \times 48 \rightarrow 1.98 \pm 0.52$

$128 \times 96 \rightarrow 2.2 \pm 0.53$

An average over all slices for both resolutions $\rightarrow 1.7 \pm 0.3$



Bodurka et al.



Resolution

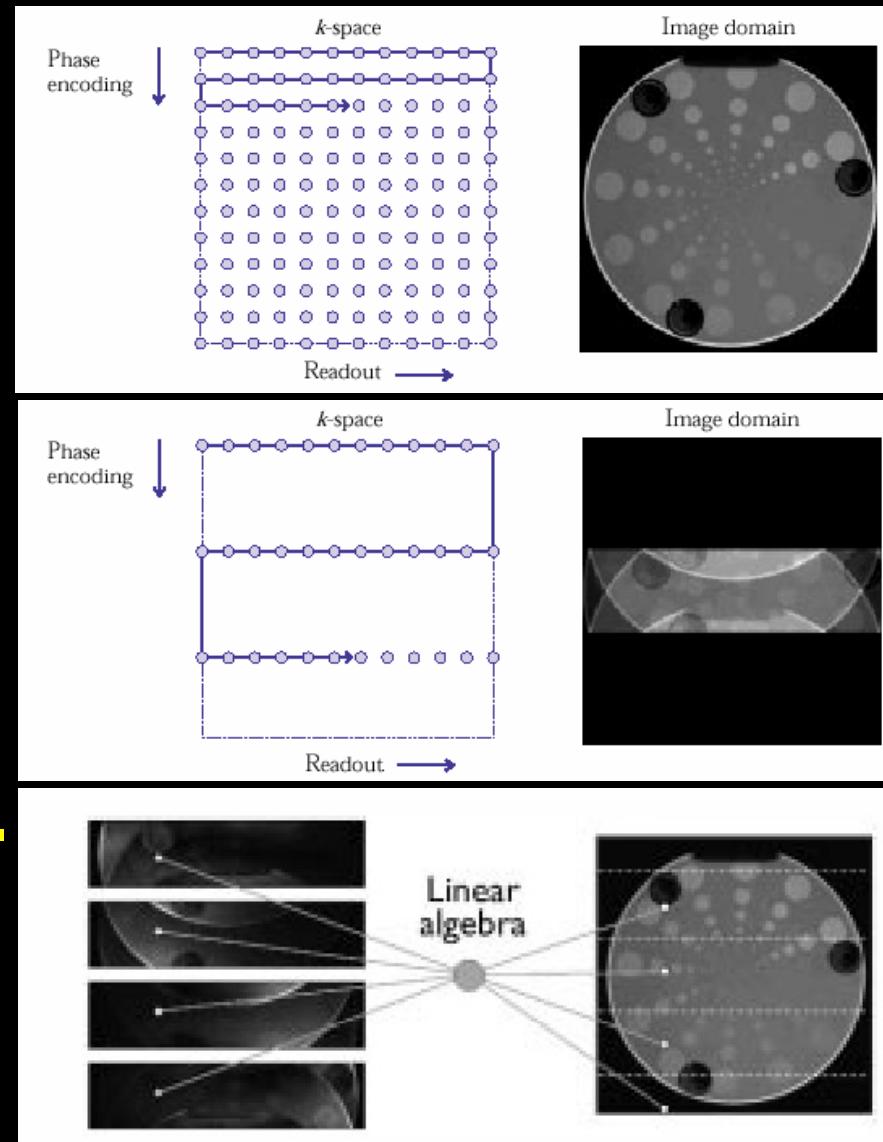
Methods to increase:

- Faster sampling rate per image
- Faster gradient switching
- Longer readout window
- Partial k-space
- Multi-shot techniques
- Parallel Imaging

Bottom Line:

- Up against limits in most methods
- Multi-shot still problematic (time, stability)
- Parallel imaging is most promising

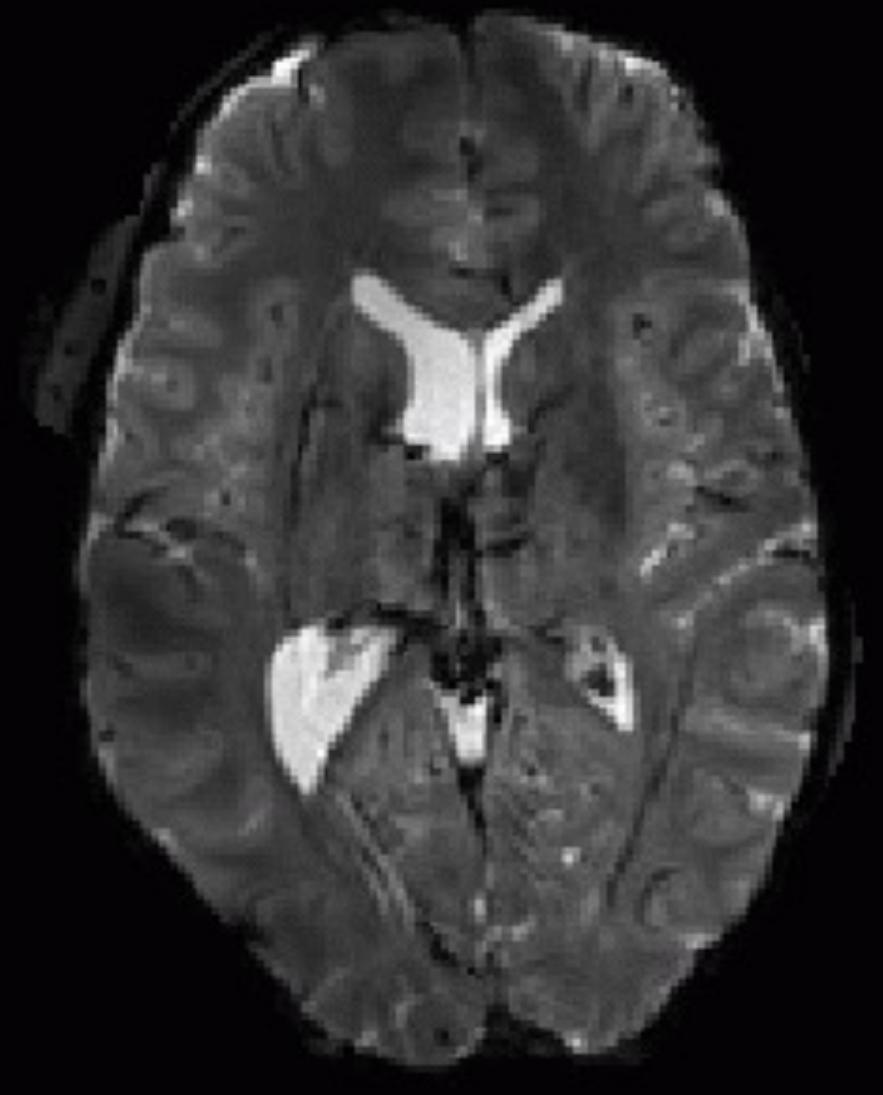
SENSE Imaging



≈ 5 to 30 ms

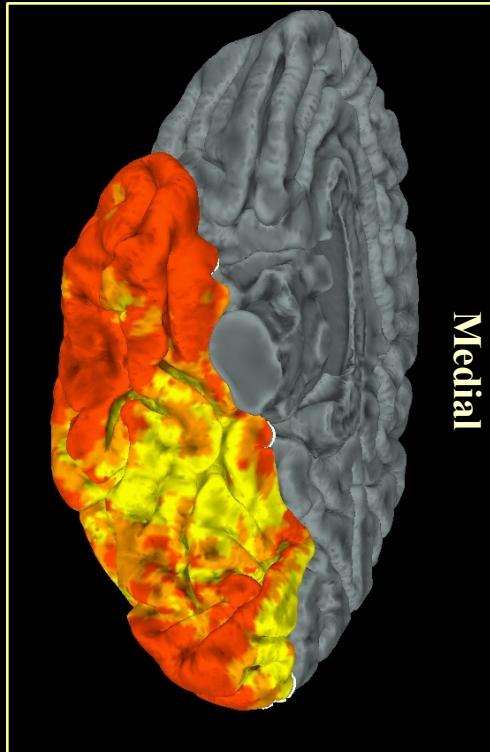
Pruessmann, et al.

Axial-oblique single
shot SENSE EPI
using 16-channel
reception. 192x144 :
1.25x1.25x2mm

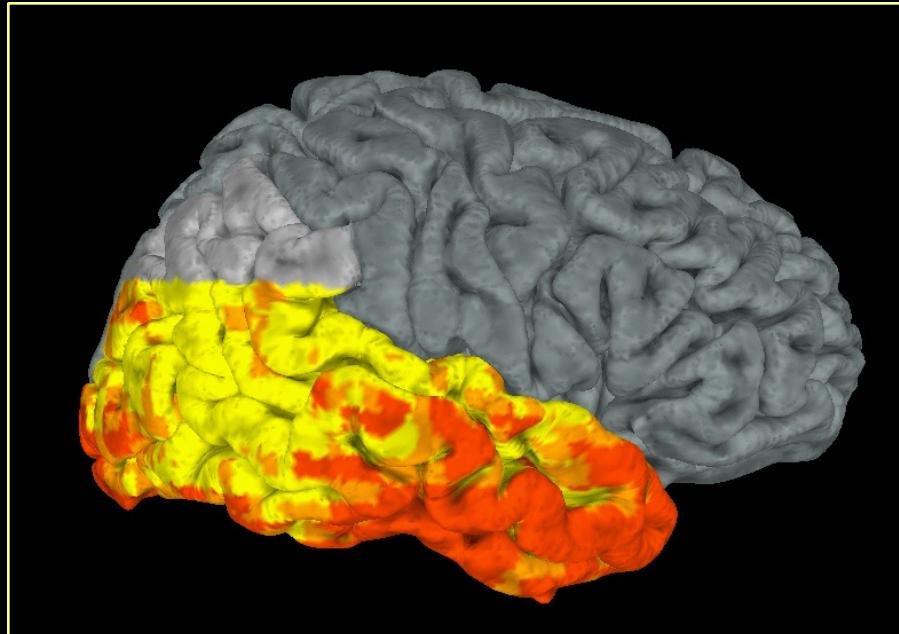


Average Temporal Signal-to-Noise ratio Comparison Between Coils

Anterior



Medial



Posterior



Shimming

A solvable problem:

- more shim coils and/or coil designs
- increased shim currents
- higher resolution (fixes dropout)
- shorter readout window (fixes distortion)
- shim inserts
- z-shim methods

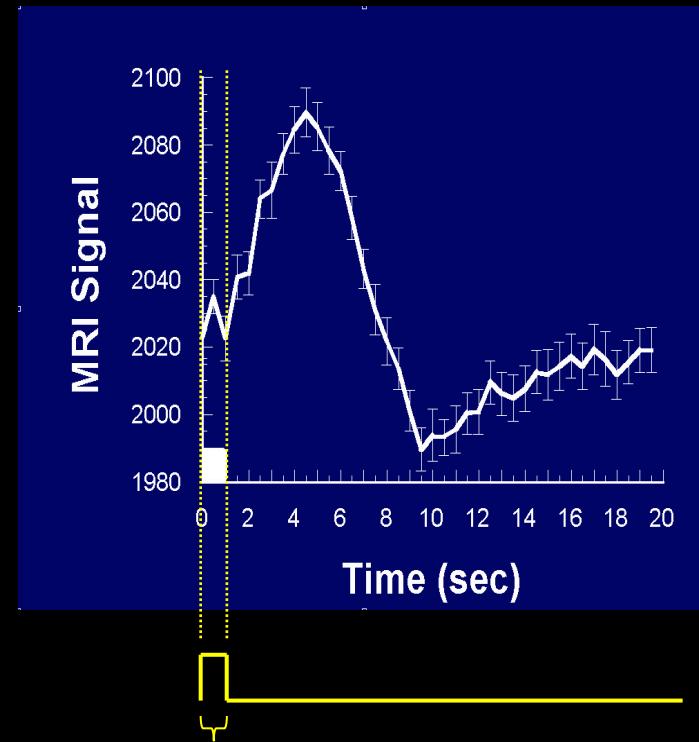
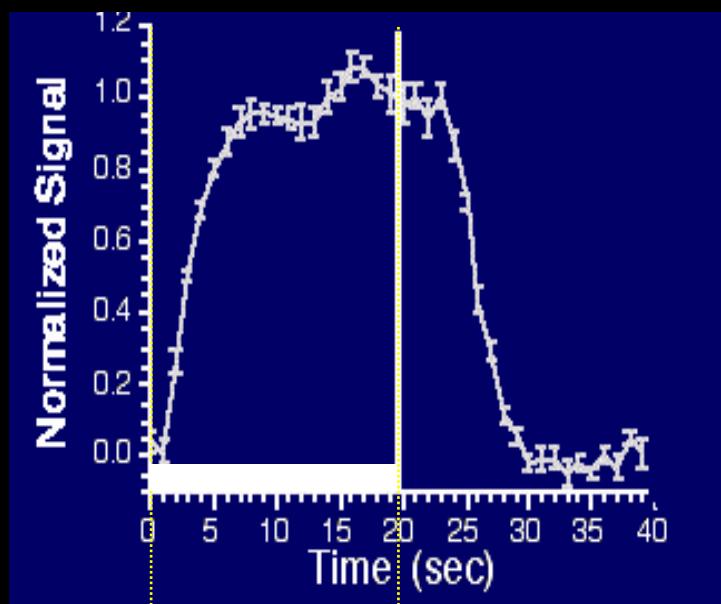
Methodology

- Temporal resolution
- Spatial specificity
- Magnitude Calibration
- Multi-subject averaging/normalization at very high resolution
- Paradigm design
- Motion (very slow and motion correlated)
- Scanner acoustic noise effect removal
- Individual Map “Classification”
- Local pattern effect mapping and classification
- Exploratory analysis techniques (ICA, PCA..)
- Temporal fluctuations (removal and use)
- Simultaneous measures with fMRI
- Baseline susceptibility mapping
- Non-invasive blood volume imaging
- Multimodal integration
- Functional Connectivity mapping
- Real time fMRI
- Neuronal Current MRI

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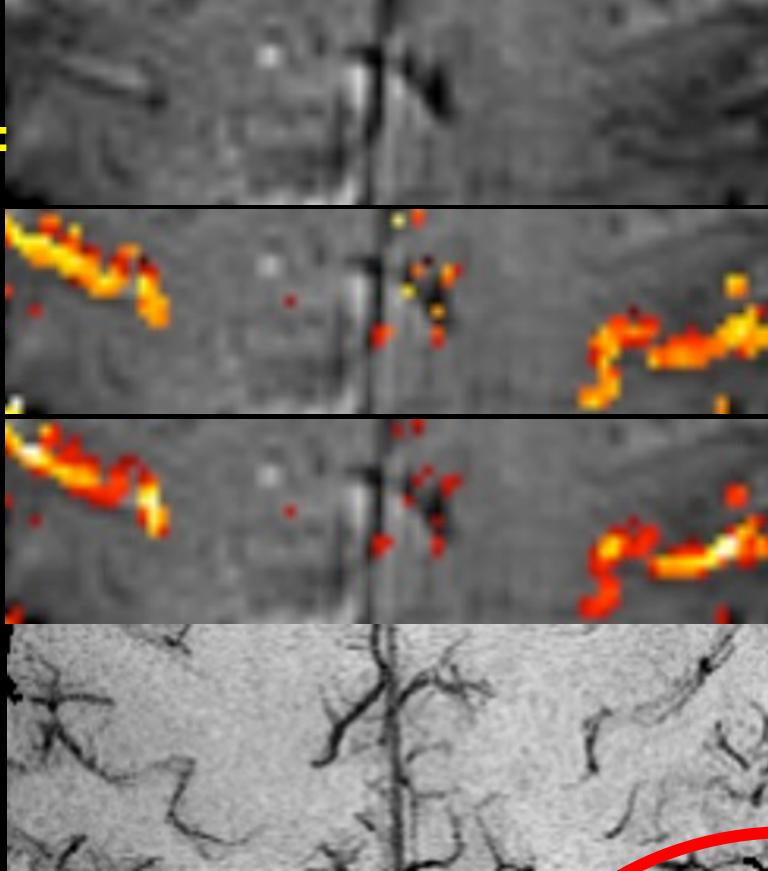
Temporal resolution



task

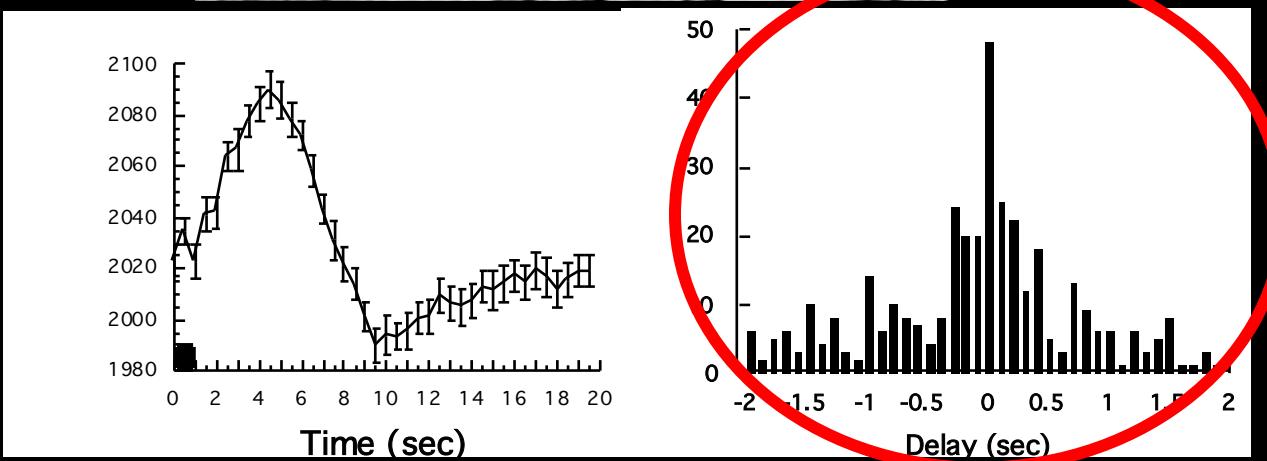
The major obstacle in BOLD contrast temporal resolution:

Latency

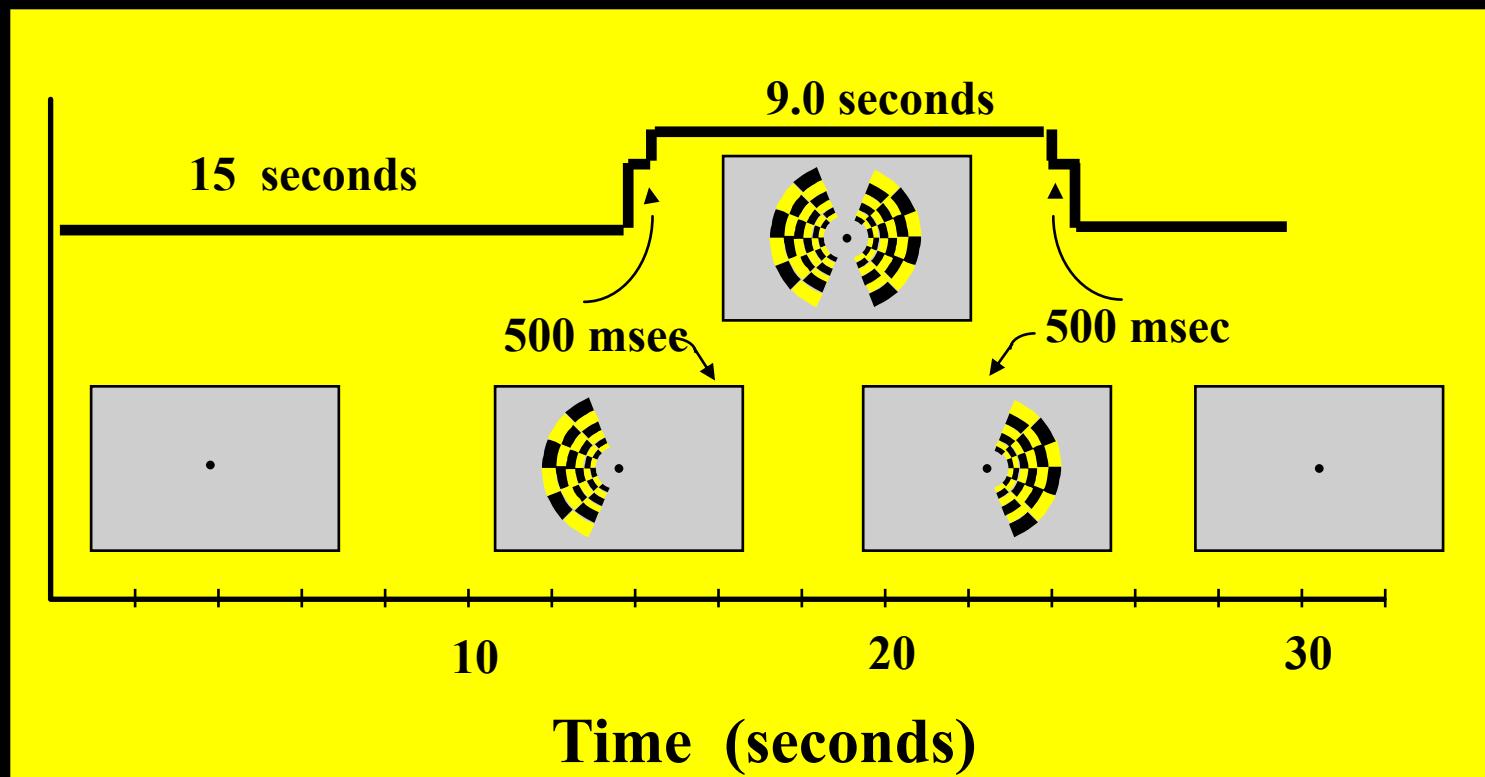
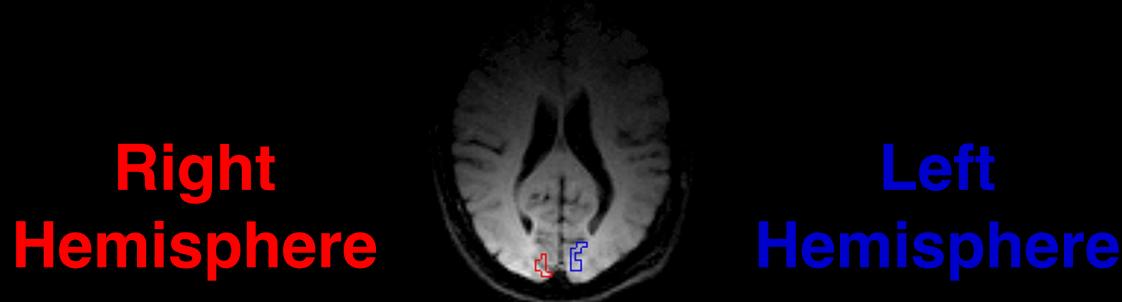


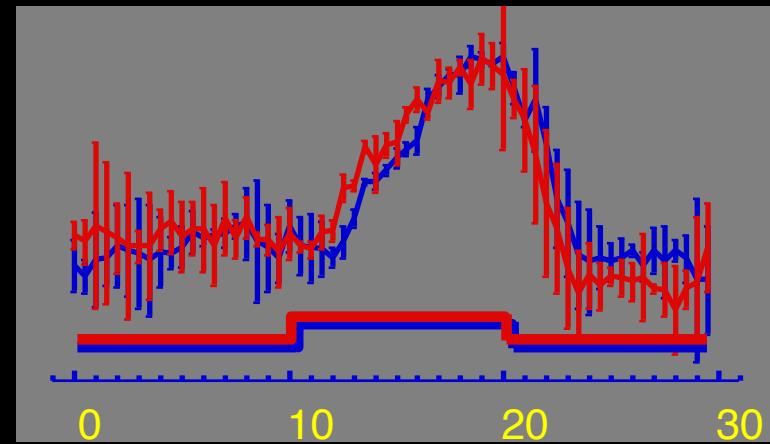
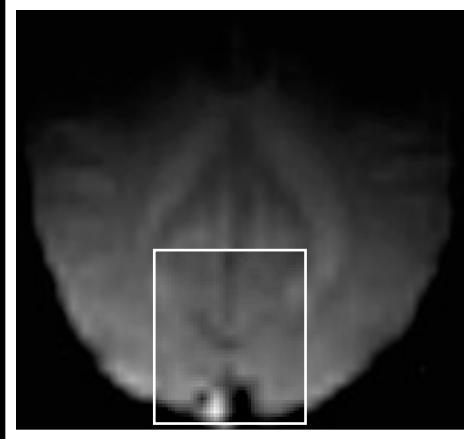
+ 2 sec
- 2 sec

Venogram



Hemi-Field Experiment





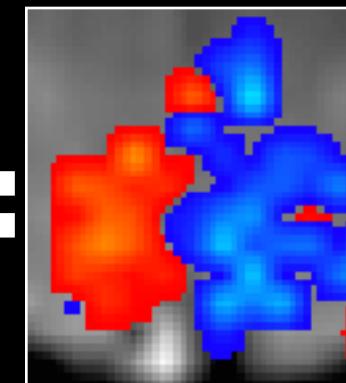
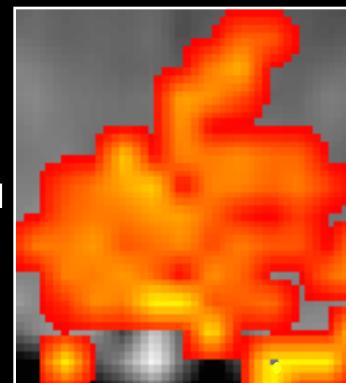
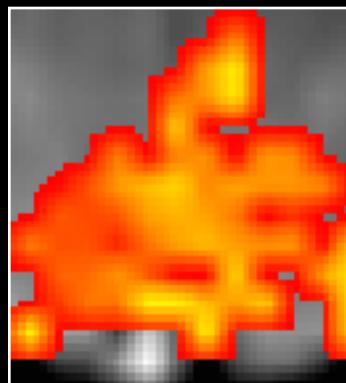
500 ms
II



500 ms
II



Right Hemifield
Left Hemifield



Cognitive Neuroscience Application:

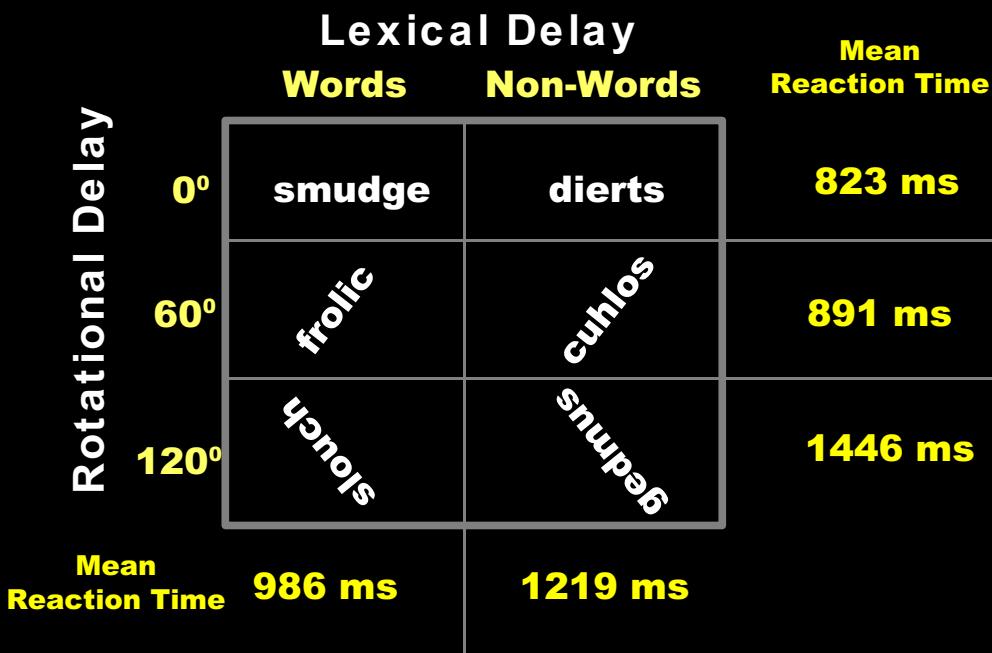
Understanding neural system dynamics through task modulation and measurement of functional MRI amplitude, latency, and width

PNAS

P. S. F. Bellgowan*,†, Z. S. Saad‡, and P. A. Bandettini*

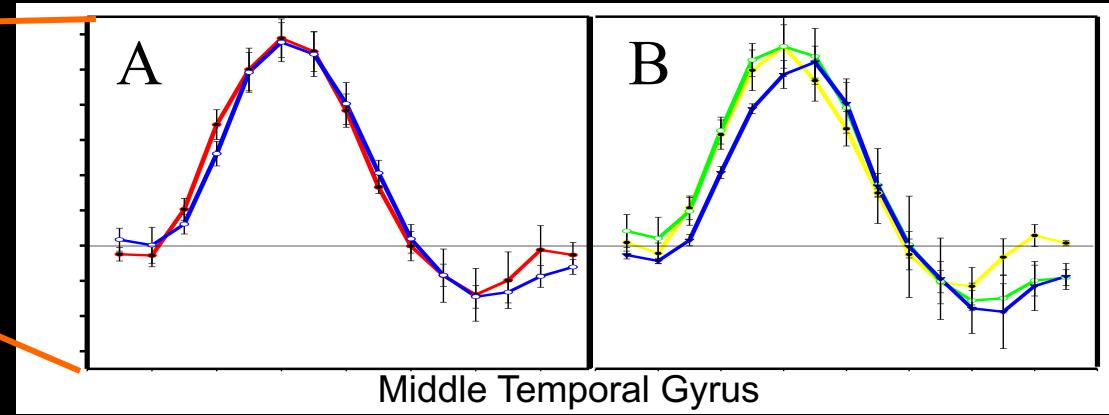
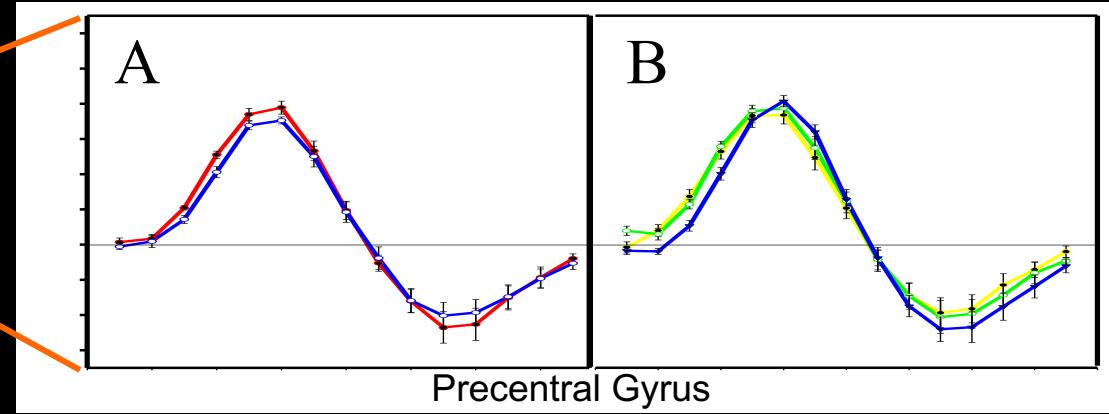
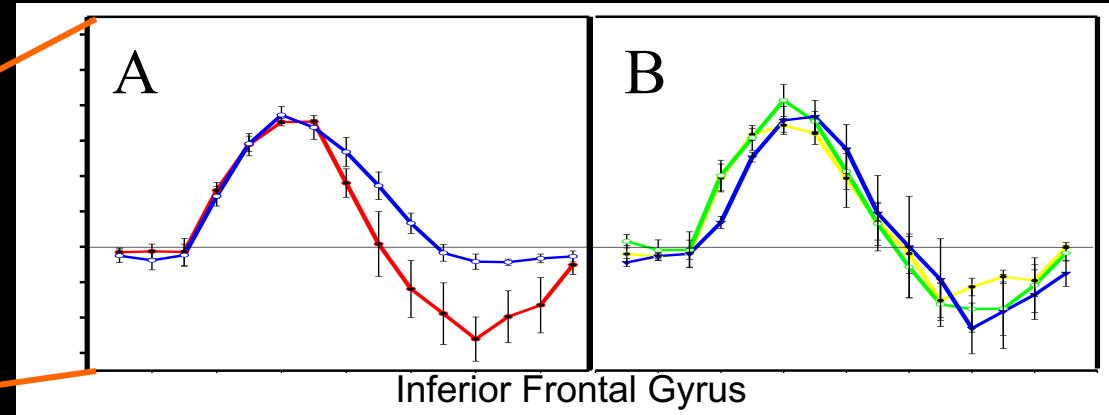
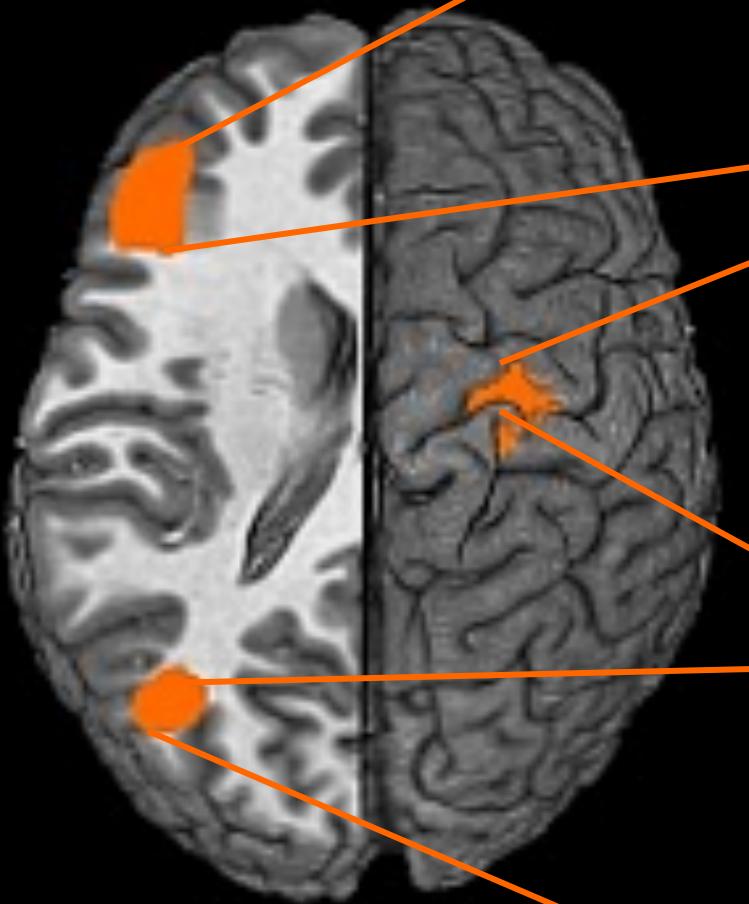
*Laboratory of Brain and Cognition and ‡Scientific and Statistical Computing Core, National Institute of Mental Health, Bethesda, MD 20892

Communicated by Leslie G. Ungerleider, National Institutes of Health, Bethesda, MD, December 19, 2002 (received for review October 31, 2002)



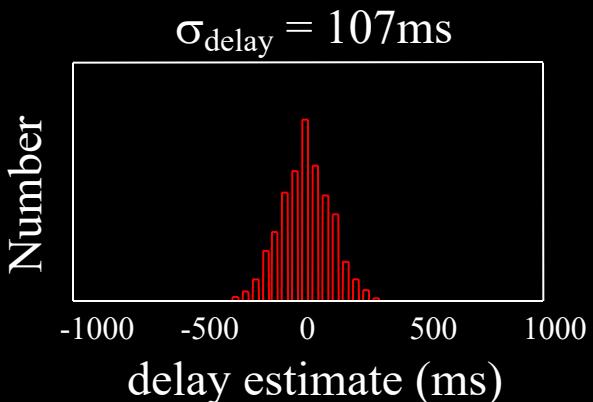
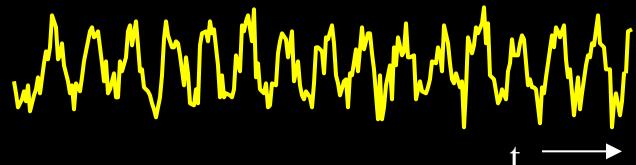
Word vs. Non-word 0°, 60°, 120° Rotation

Regions of Interest

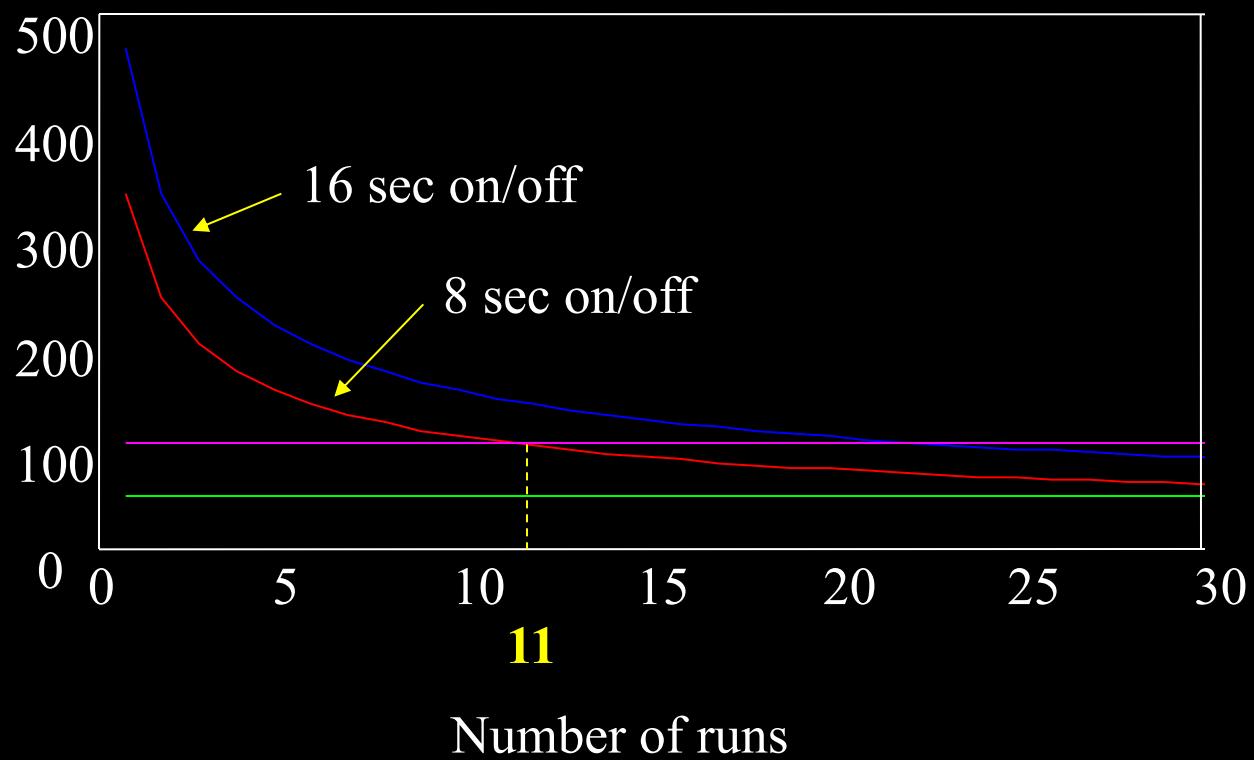


1 run:

1% Noise
4% BOLD
256 time pts /run
1 second TR



Smallest latency
Variation Detectable
(ms) ($p < 0.001$)



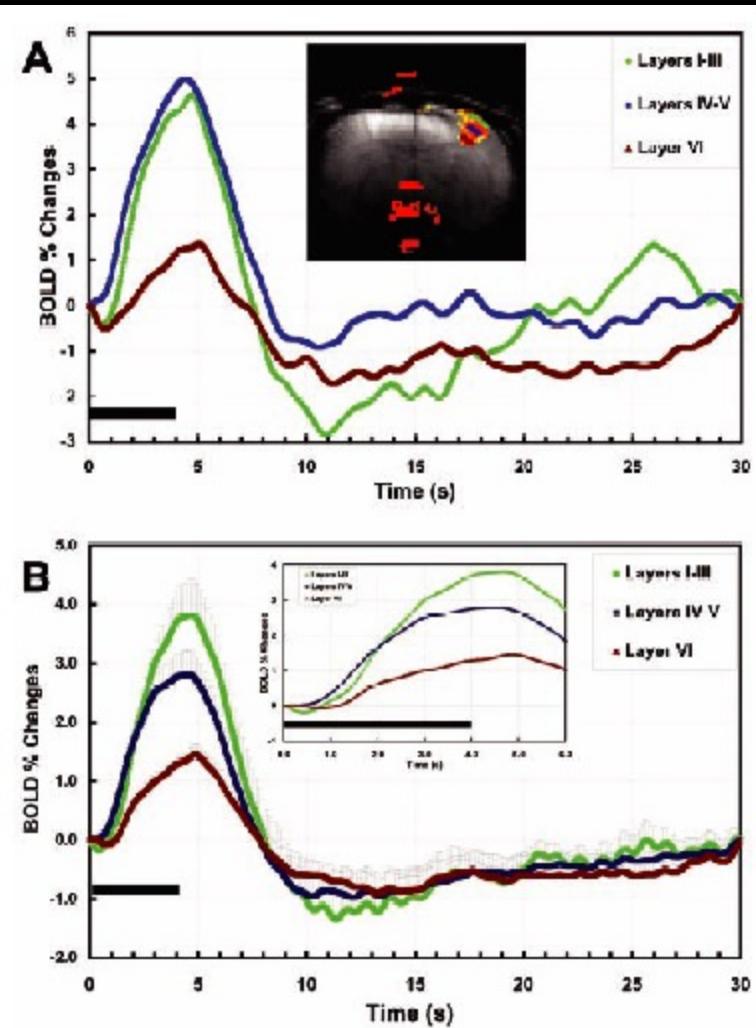
Laminar specificity of functional MRI onset times during somatosensory stimulation in rat

Afonso C. Silva* and Alan P. Koretsky

Laboratory of Functional and Molecular Imaging, National Institute of Neurological Disorders and Stroke, Bethesda, MD 20892

15182–15187 | PNAS | November 12, 2002 | vol. 99 | no. 23

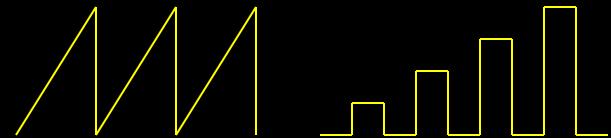
No calibration



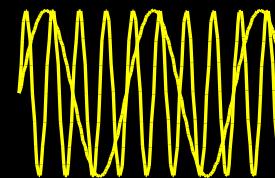
11.7 T

Paradigm Design

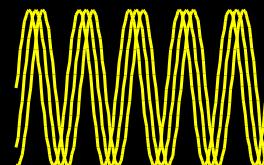
1. Block Design



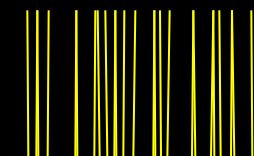
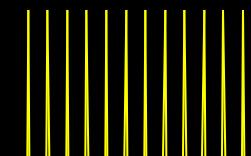
2. Parametric Design



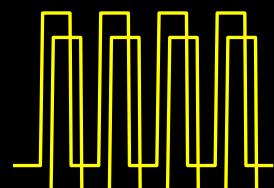
3. Frequency Encoding



4. Phase Encoding



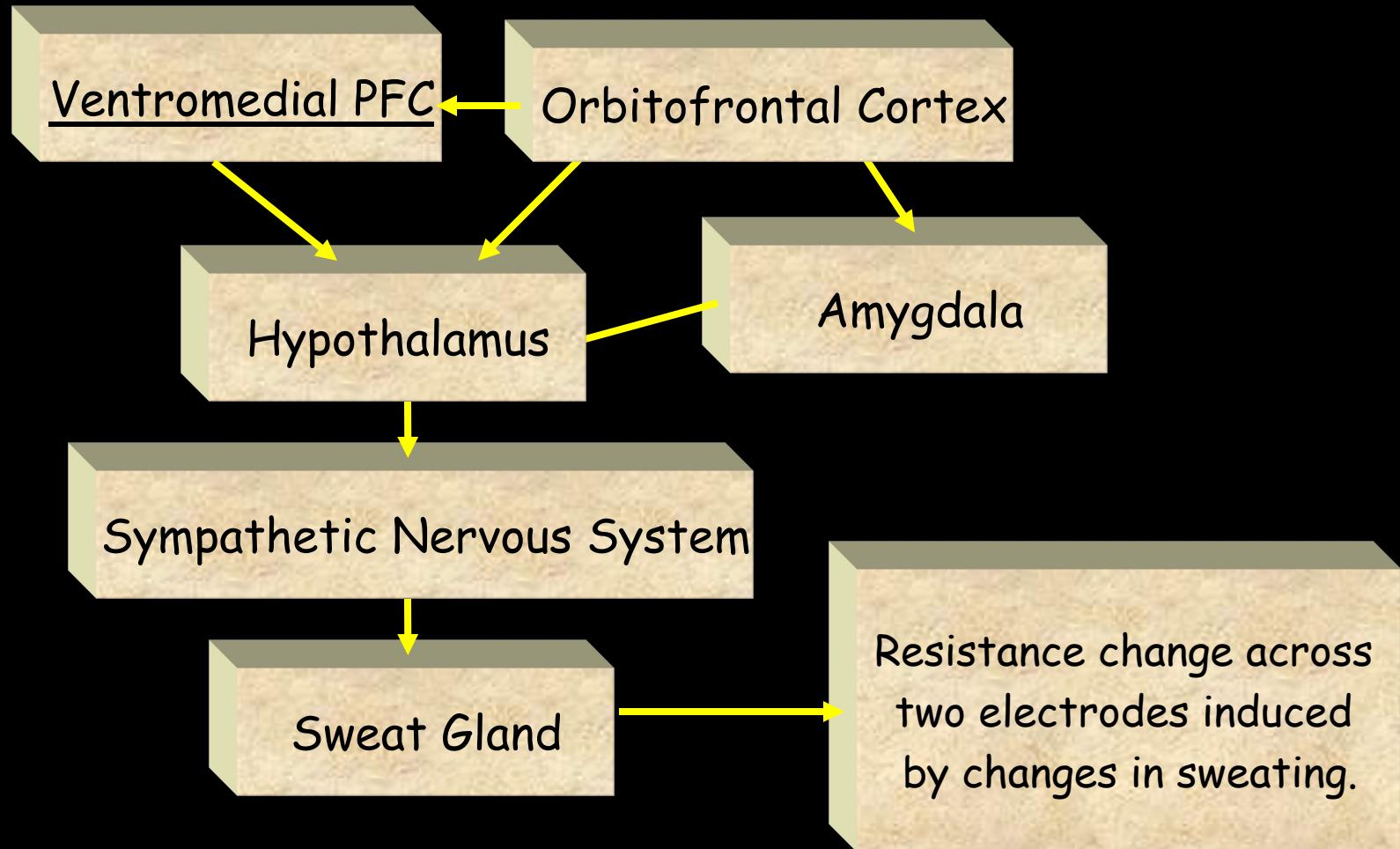
5. Event Related



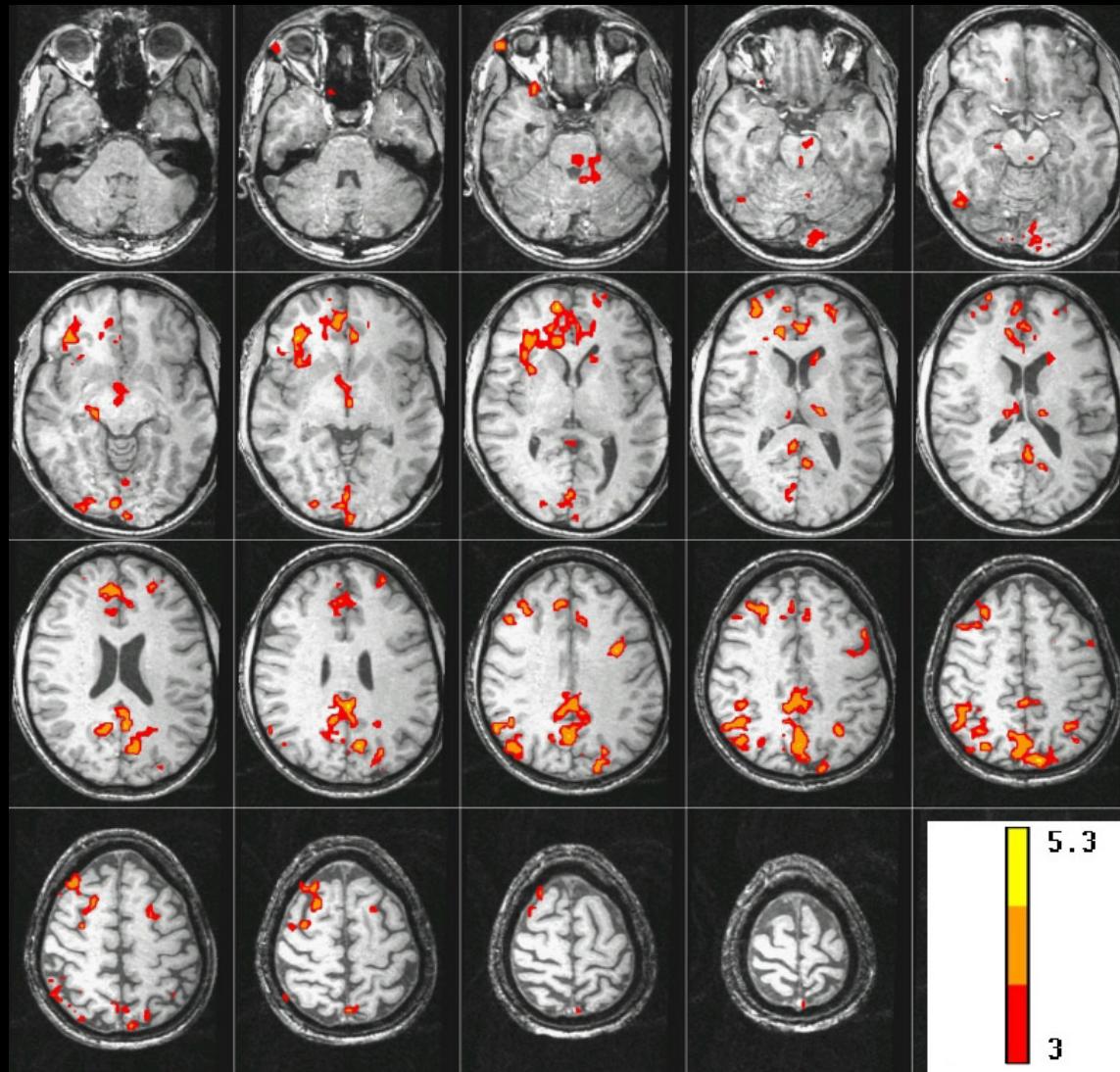
6. Orthogonal Design

7. Free Behavior Design

The Skin Conductance Response (SCR)



Brain activity correlated with SCR during “Rest”



J. C. Patterson II, L. G. Ungerleider, and P. A. Bandettini, Task - independent functional brain activity correlation with skin conductance changes: an fMRI study. *NeuroImage* 17: 1787-1806, (2002).

Simultaneous EEG and fMRI of the alpha rhythm

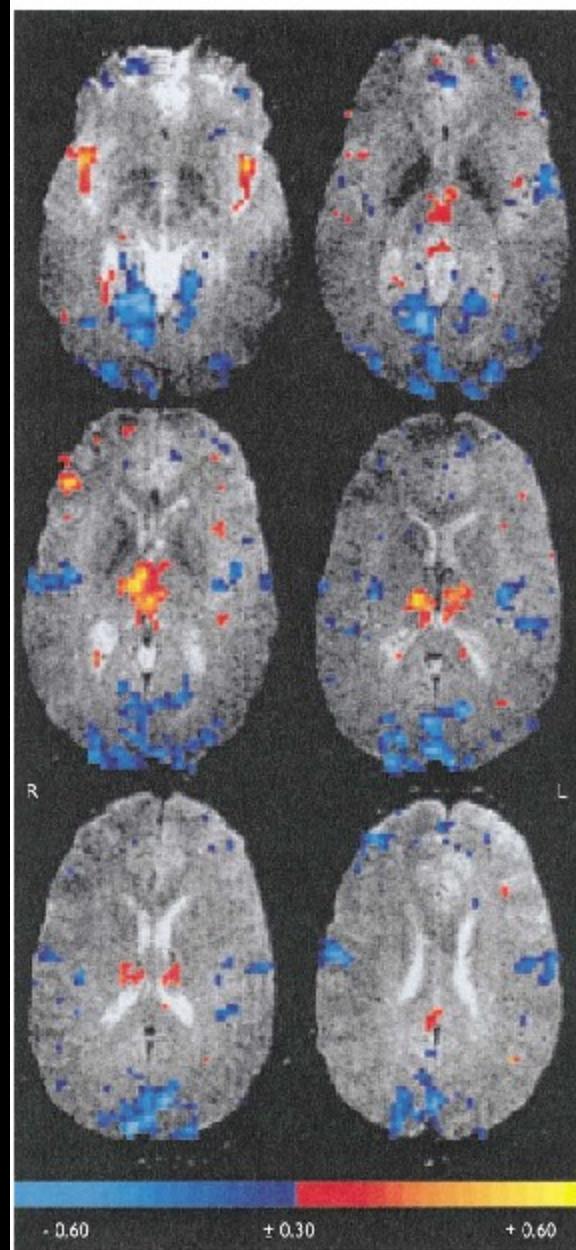
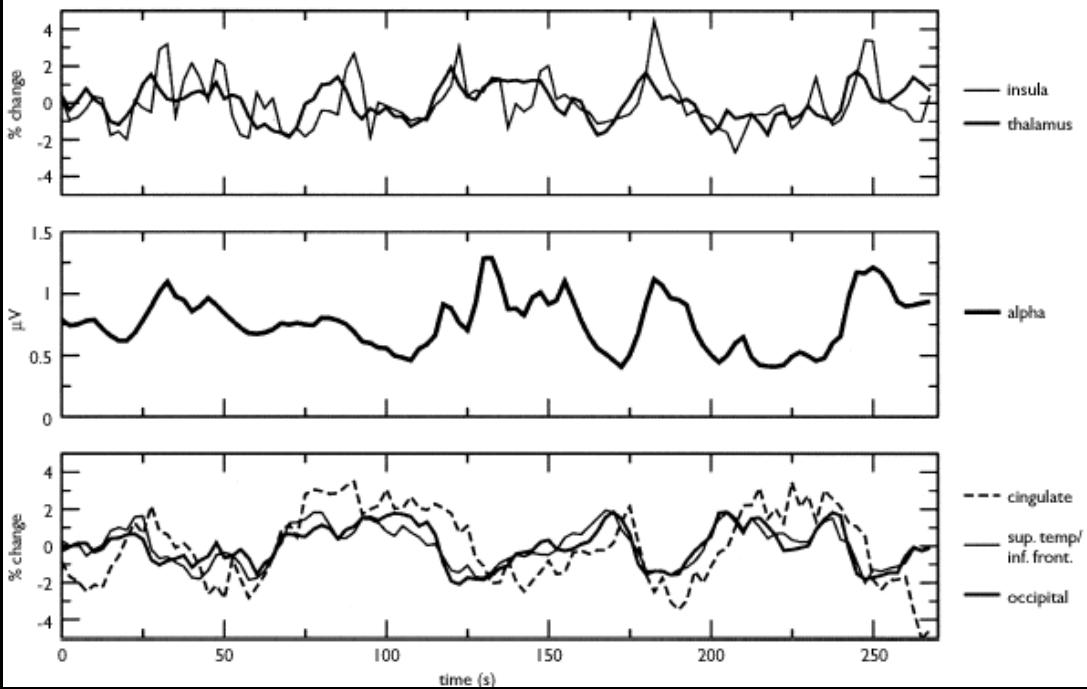
Robin I. Goldman,^{2,CA} John M. Stern,¹ Jerome Engel Jr¹ and Mark S. Cohen

Ahmanson-Lovelace Brain Mapping Center, UCLA, 660 Charles Young Drive South, Los Angeles, CA 90095; ¹Department of Neurology, UCLA School of Medicine, Los Angeles, CA; ²Hatch Center for MR Research, Columbia University, HSD, 710 W. 168th St., NIB-I, Mailbox 48, NY, NY 10032, USA

CA,²Corresponding Author and Address: rg2146@columbia.edu

Received 28 October 2002; accepted 30 October 2002

DOI: 10.1097/01.wnr.0000047685.08940.d0



Motion (very slow and activation correlated)

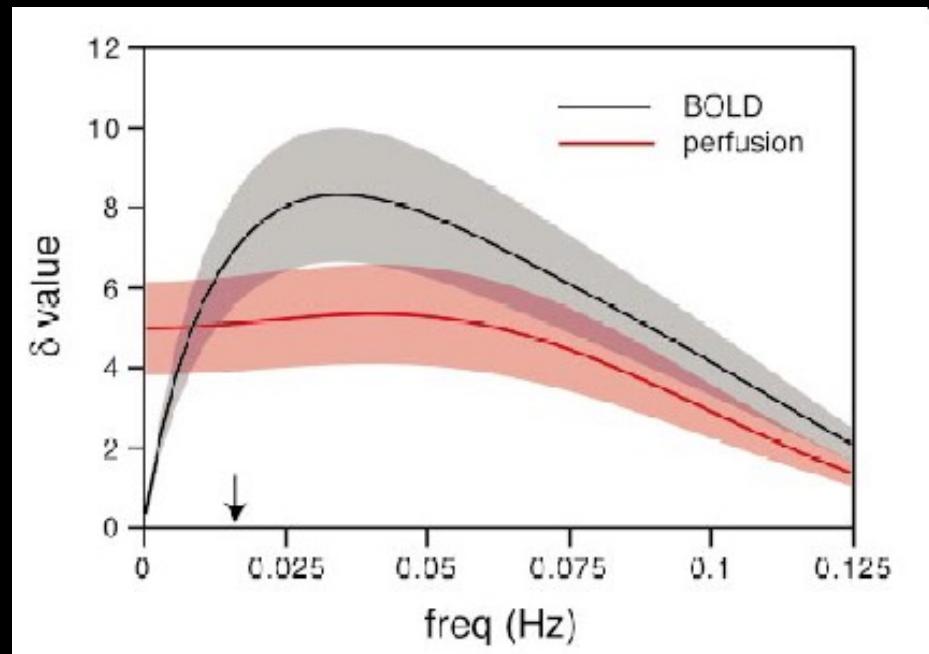
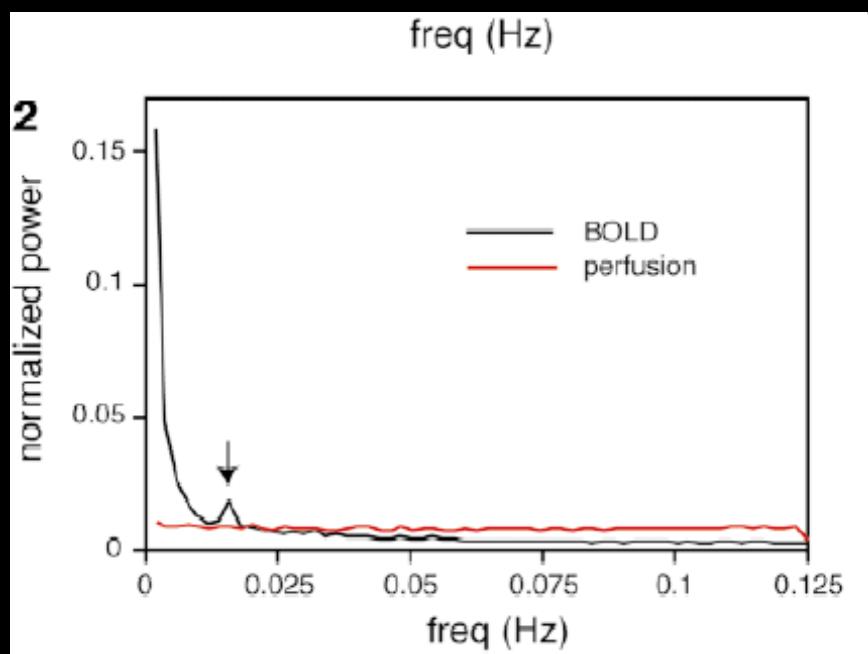
Very slow:

- a problem when looking at slow state changes
- one solution: ASL techniques

Activation correlated:

- separable from hemodynamic response

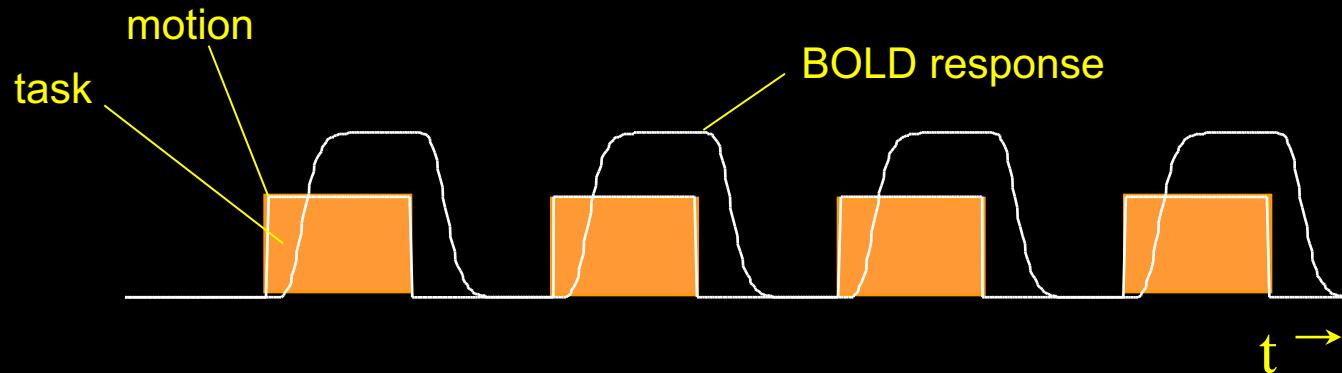
ASL Techniques show more temporal stability



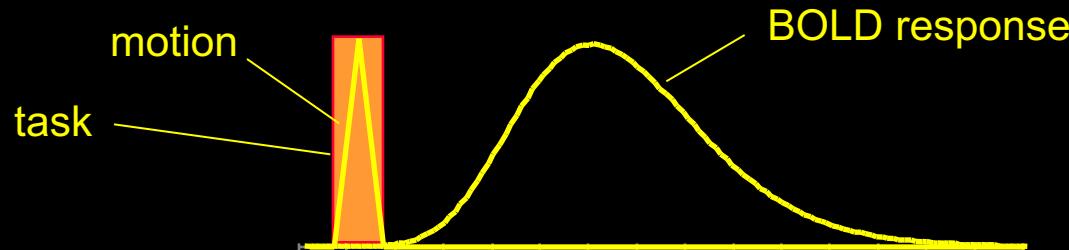
Experimental design and the relative sensitivity of BOLD and perfusion fMRI Aguirre GK, Detre JA, Zarahn E, Alsop DC, NEUROIMAGE 15 (3): 488-500 MAR 2002

fMRI during tasks that involve brief motion

Blocked Design

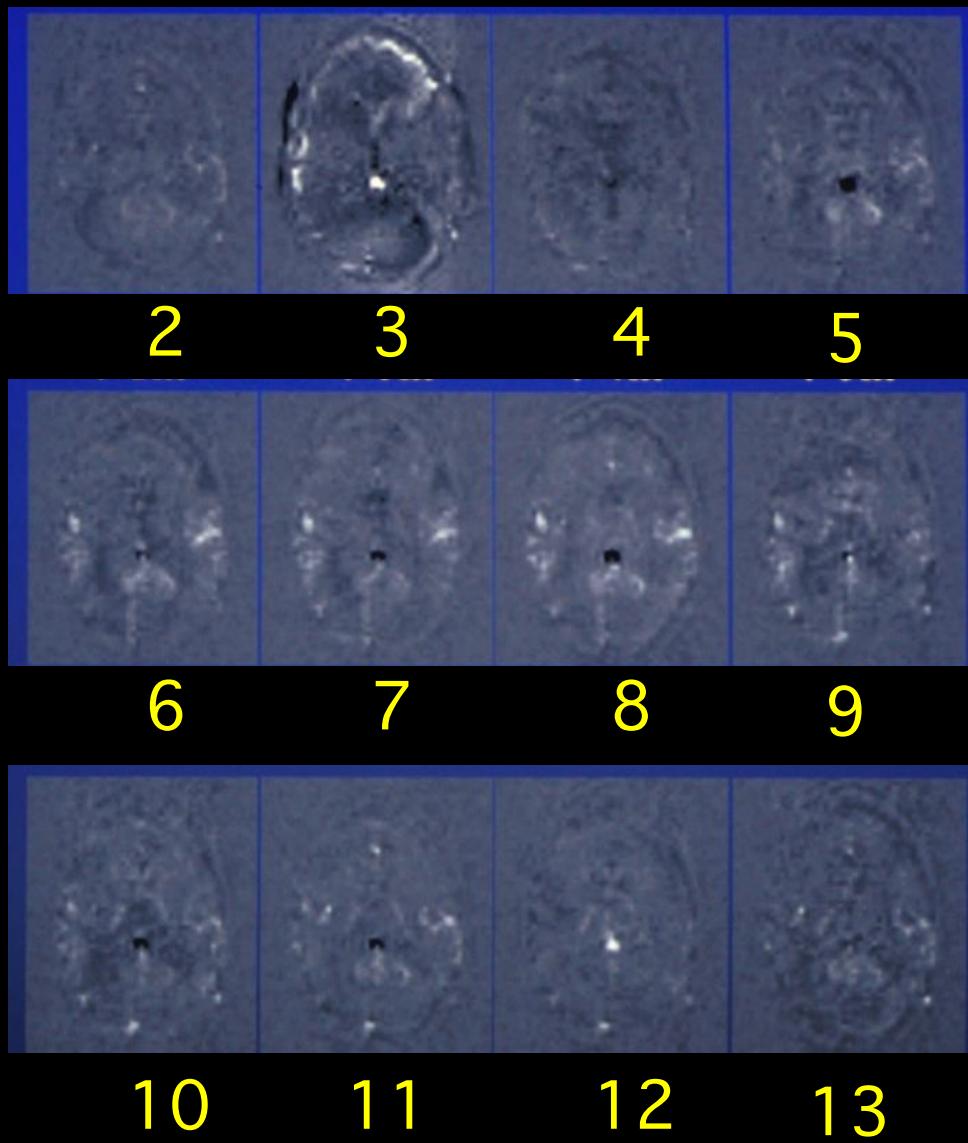


Event-Related Design



R. M. Birn, P. A. Bandettini, R. W. Cox, R. Shaker, Event - related fMRI of tasks involving brief motion. *Human Brain Mapping* 7: 106-114 (1999).

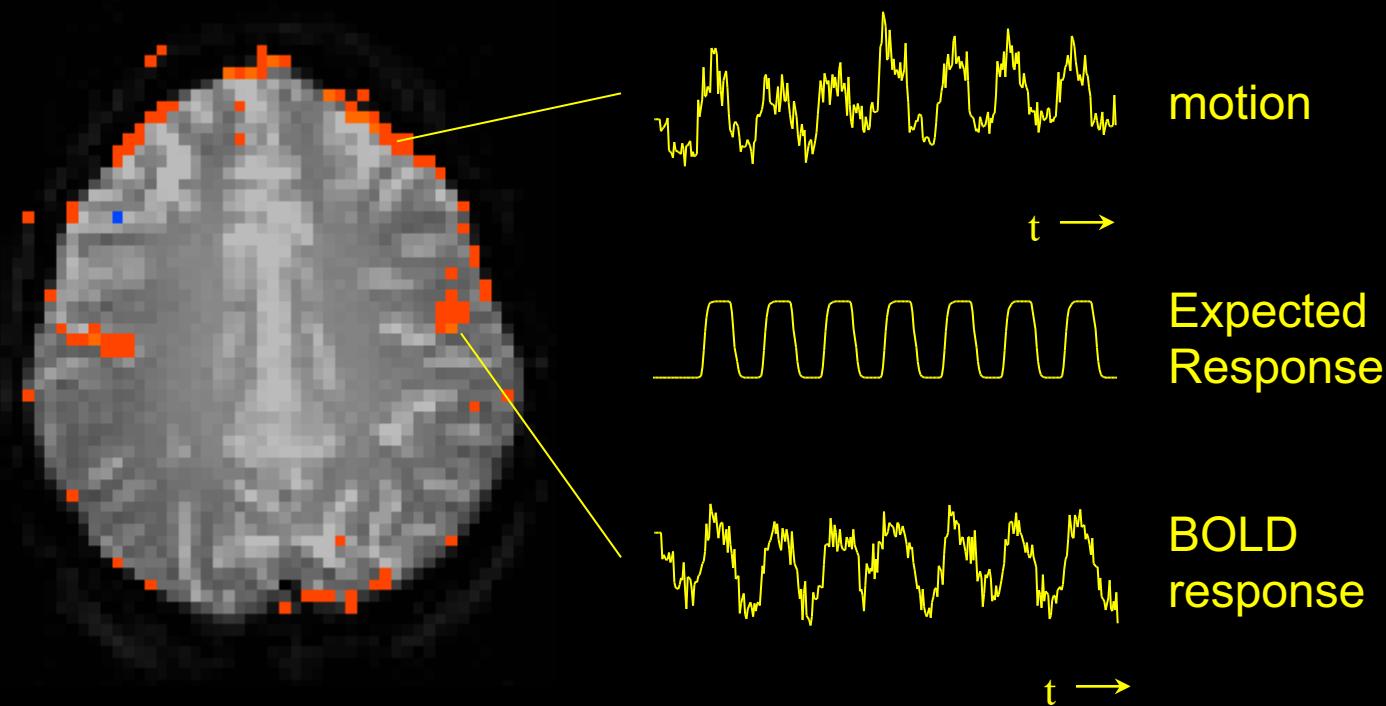
Overt Word Production



R. M. Birn, P. A. Bandettini, R. W. Cox, R. Shaker, Event - related fMRI of tasks involving brief motion. *Human Brain Mapping* 7: 106-114 (1999).

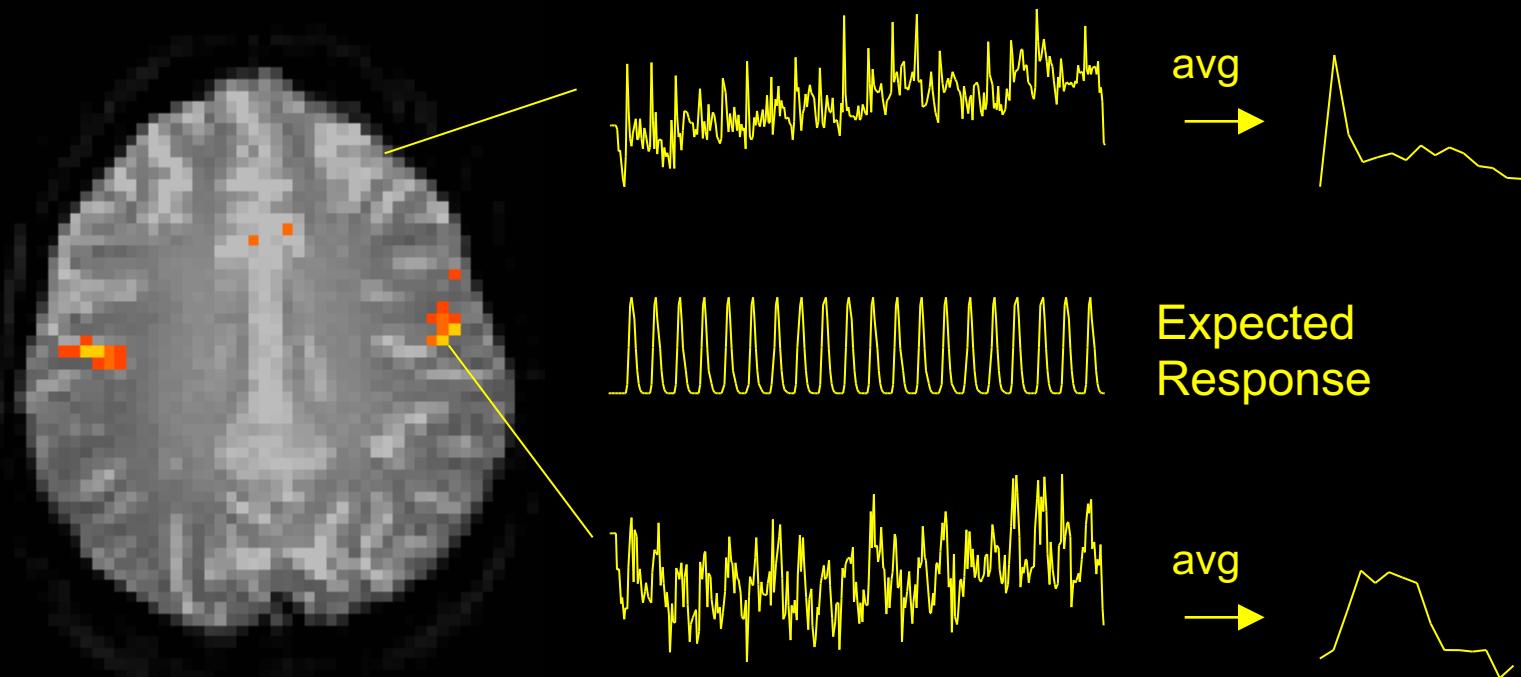
Speaking – Blocked design

R.M. Birn, et al. *Human Brain Mapping* 7(2), 106-114, 1999



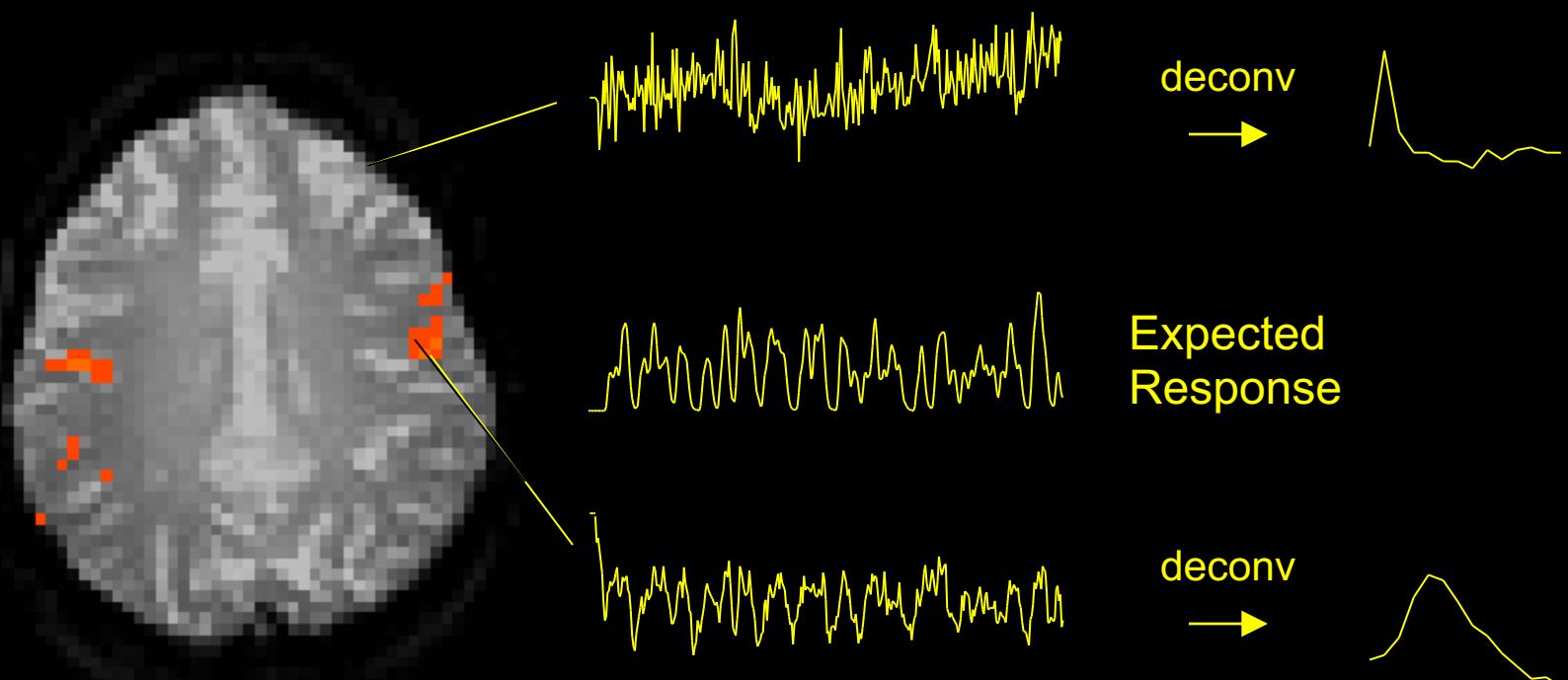
Constant ISI Speaking – Event related design

R.M. Birn, et al. *Human Brain Mapping* 7(2), 106-114, 1999



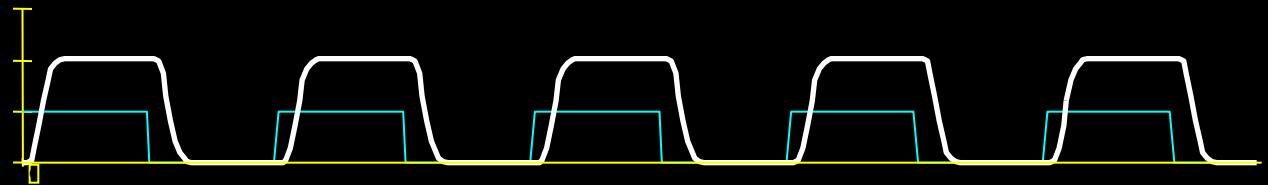
Variable ISI

Speaking - ER-fMRI

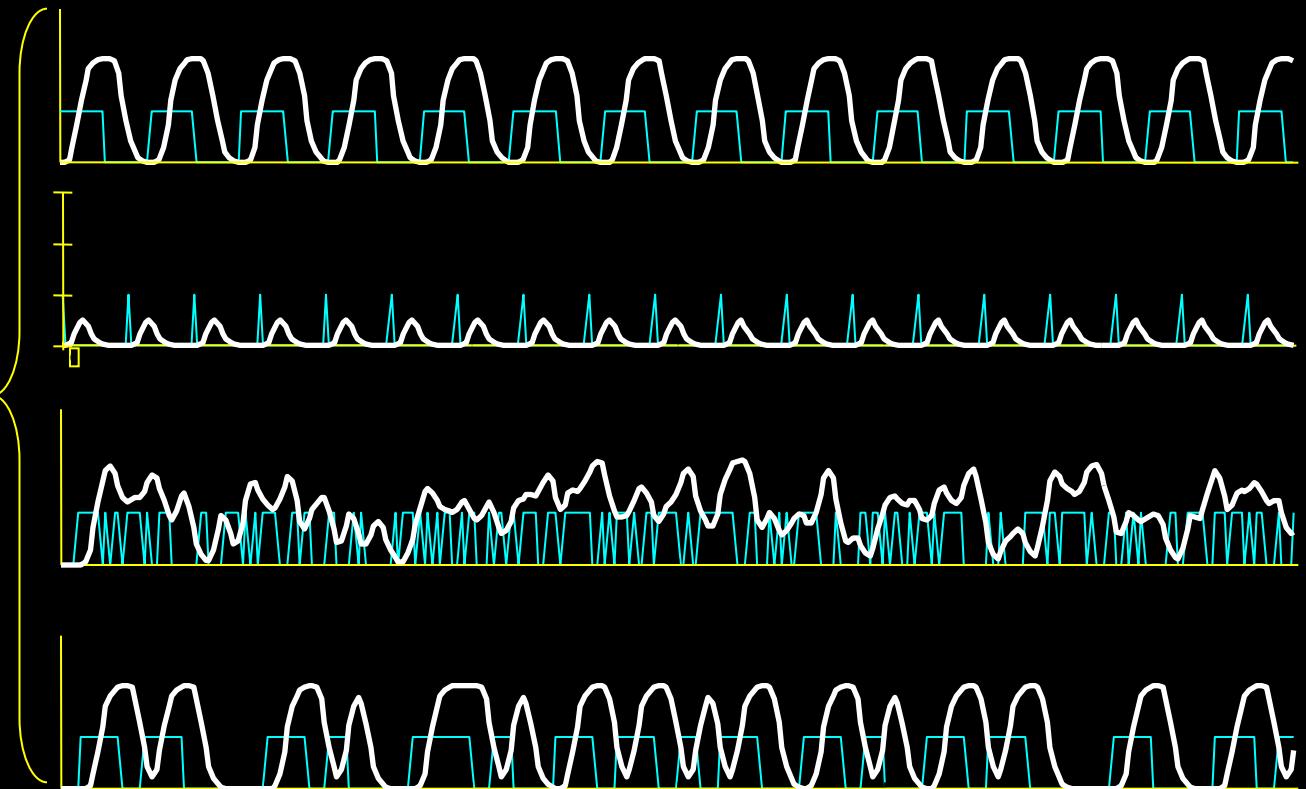


Optimizing the stimulus paradigm

Blocked
(motion highly correlated)

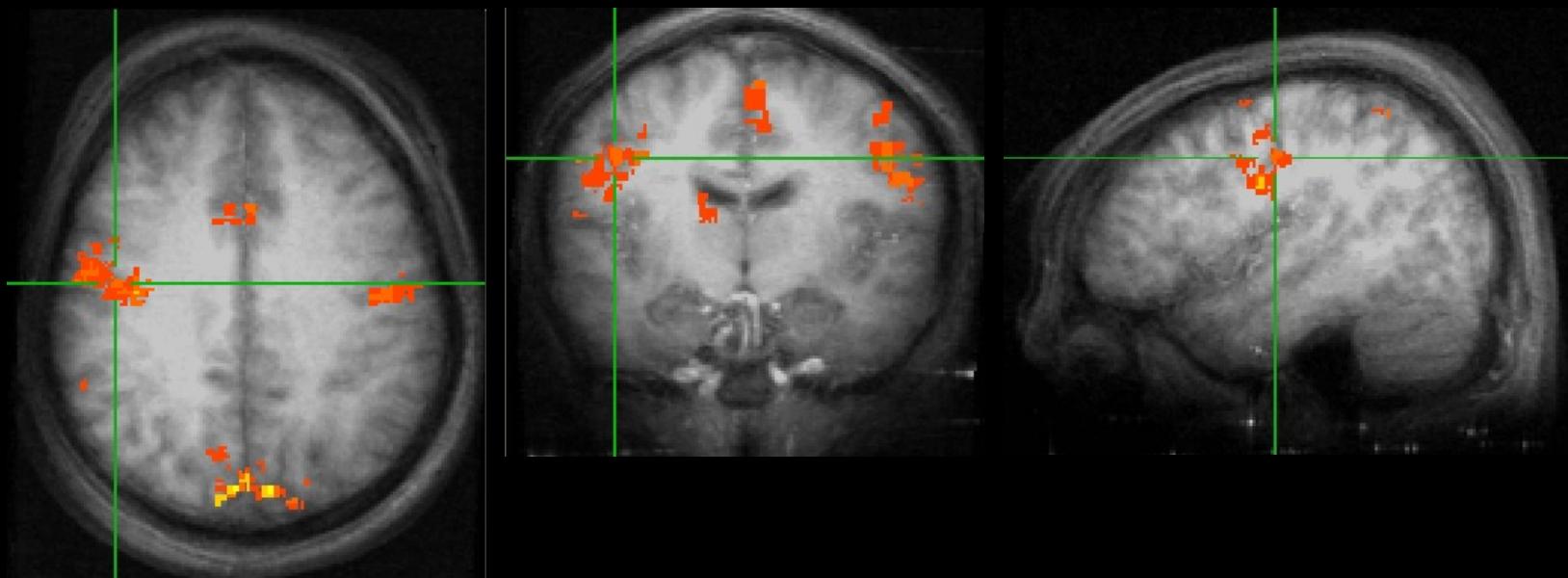


Blocked /
Event-Related
(low correlation
w/ motion)



Swallowing - Event-Related

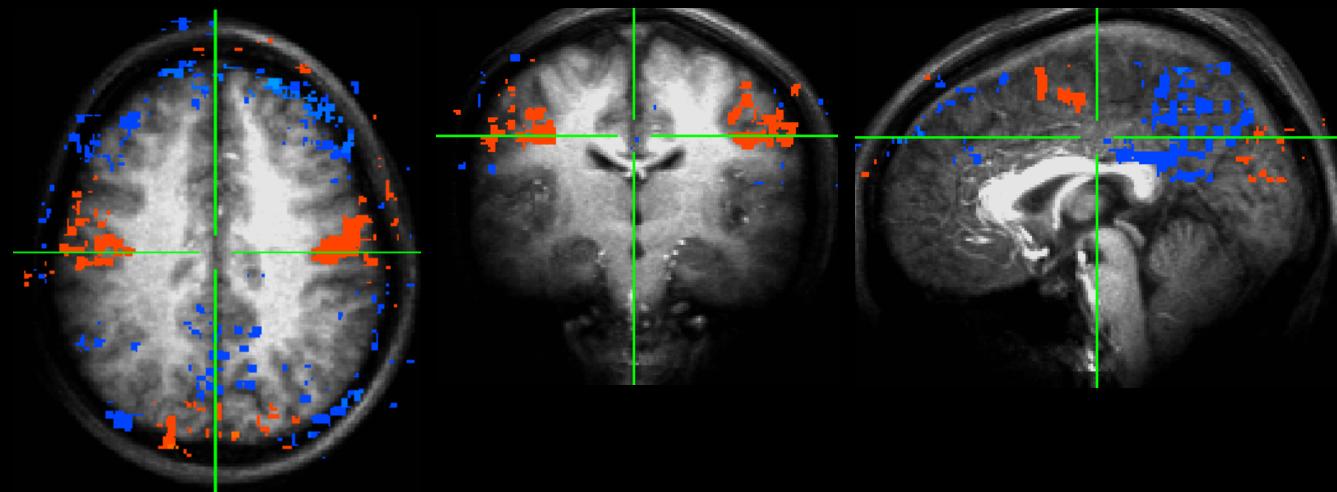
M.K. Kern, R.M. Birn, S. Jaradeh, et al., Am J Physiol Gastrointest Liver Physiol, 280(4), G531-538, 2001.



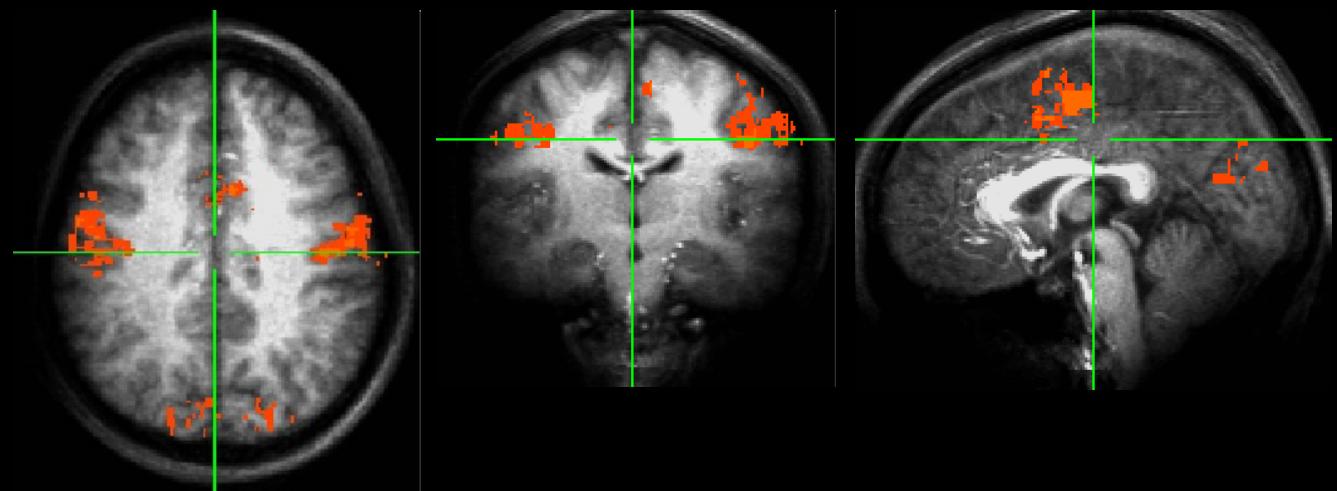
Facial muscle movement

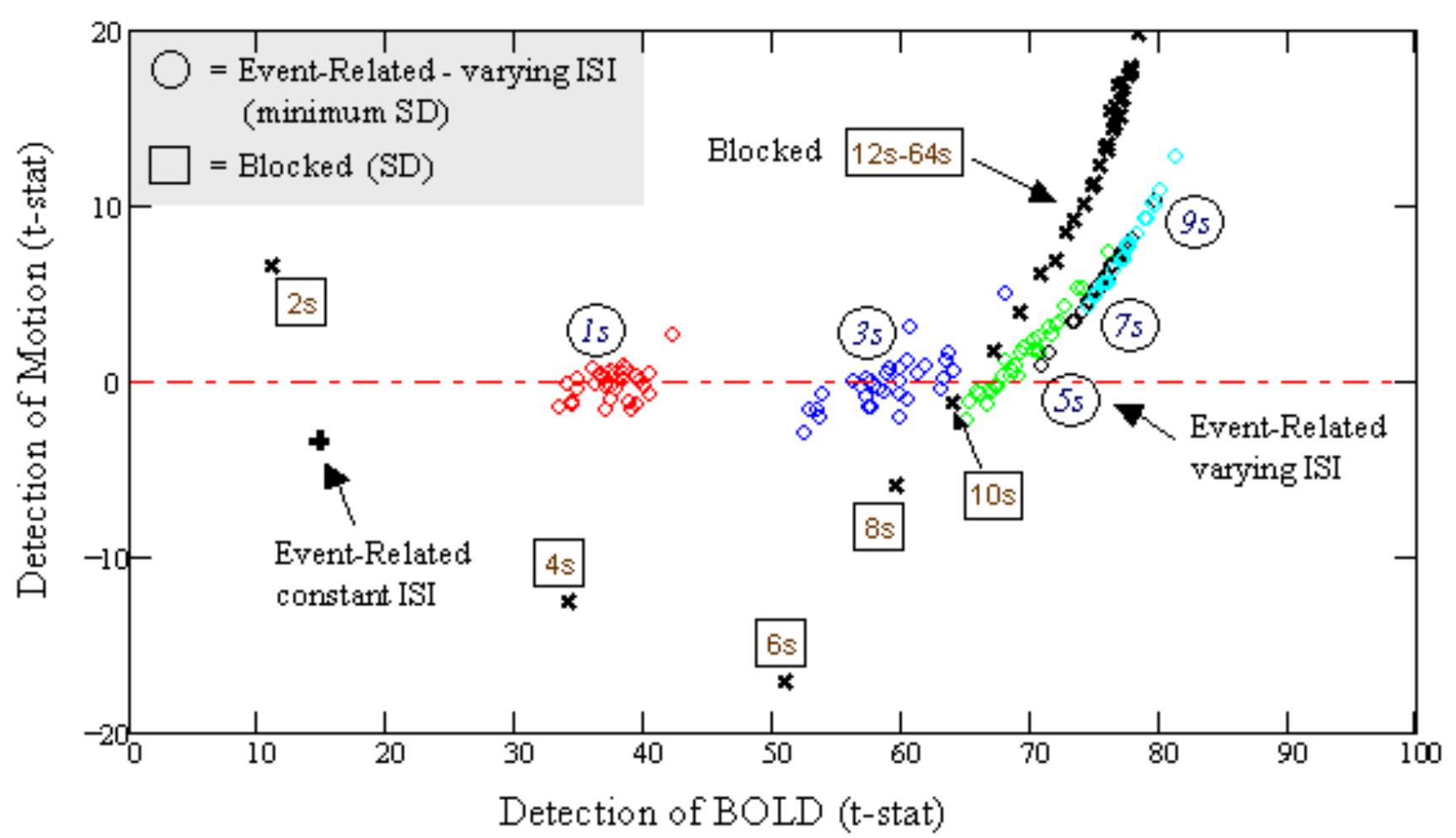
R.M. Birn, et al. *Human Brain Mapping* 7(2), 106-114, 1999

Blocked
design



Event -
Related
design



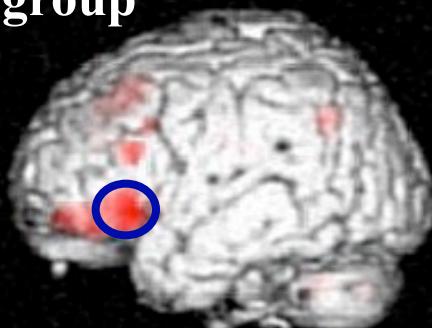


Individual Map “Classification”

The issue: We can make inferences about groups when averaging individual maps, but can we make inferences which group an individual belongs to?

Not yet. Requires extensive classification techniques.

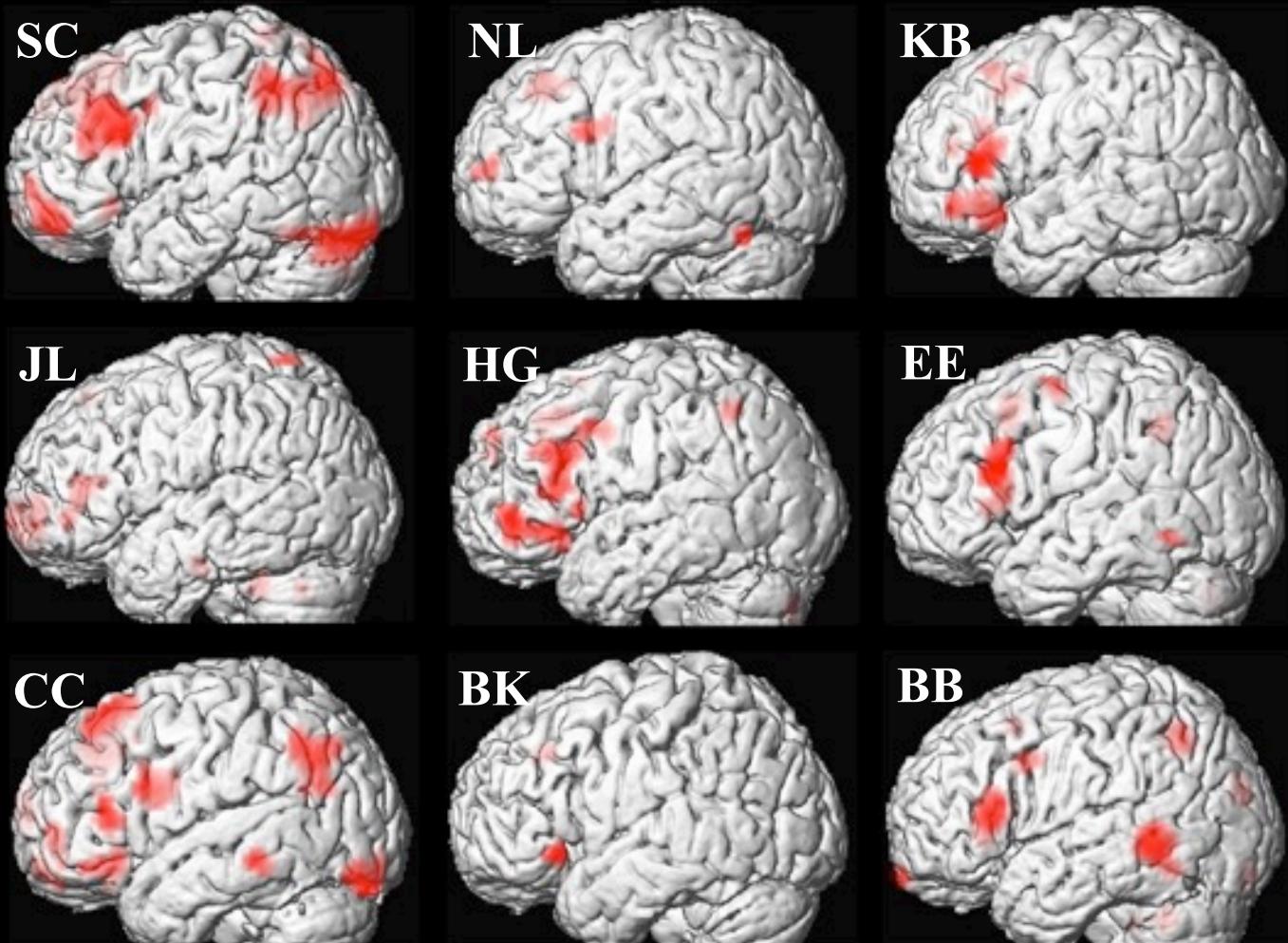
group



Extensive Individual Differences in Brain Activations During Episodic Retrieval

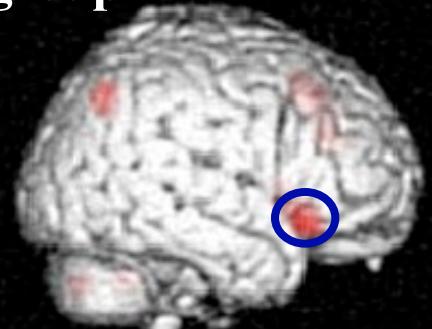
Miller et al., 2002

Individual activations from the left hemisphere of the 9 subjects



Courtesy, Mike Miller, UC
Santa Barbara and Jack Van
Horn, fMRI Data Center,
Dartmouth University

group

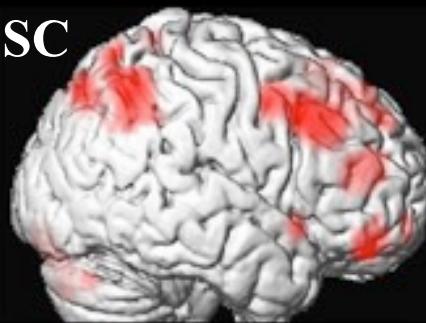


Extensive Individual Differences in Brain Activations During Episodic Retrieval

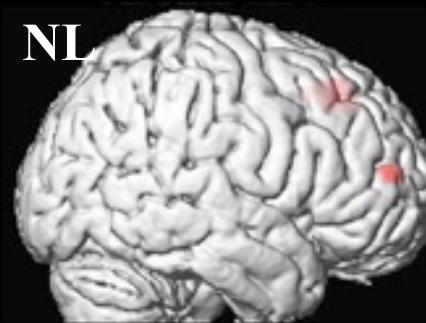
Miller et al., 2002

Individual activations from the right hemisphere of the 9 subjects

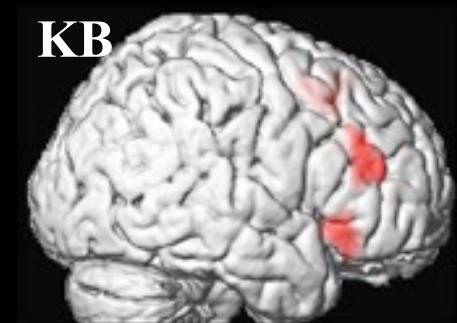
SC



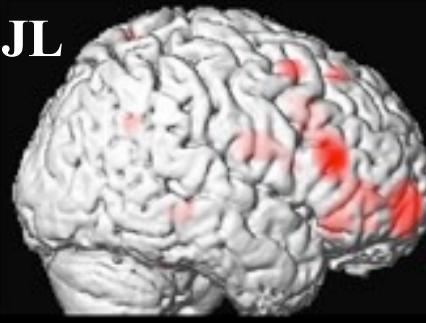
NL



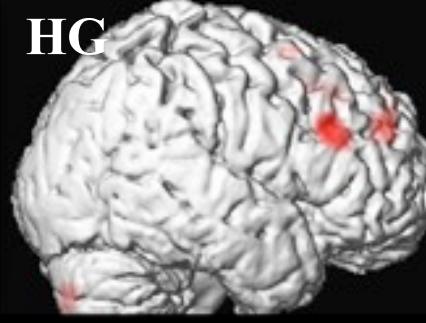
KB



JL



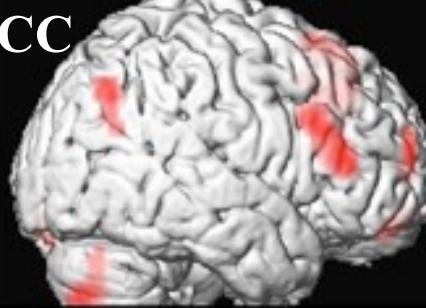
HG



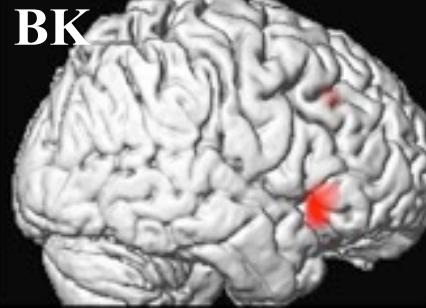
EE



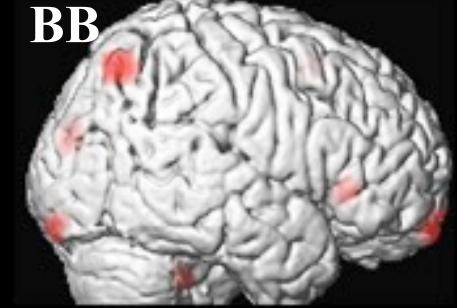
CC



BK

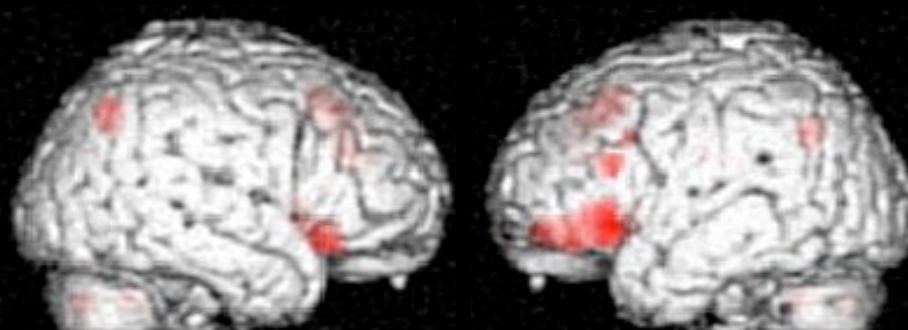


BB



Courtesy, Mike Miller, UC
Santa Barbara and Jack Van
Horn, fMRI Data Center,
Dartmouth University

These individual patterns of activations are stable over time



Group Analysis of Episodic Retrieval



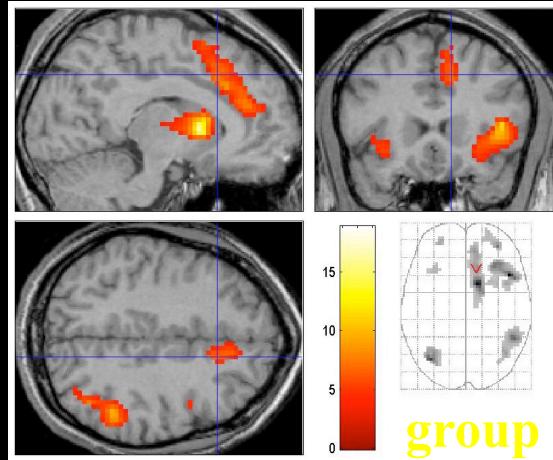
Subject SC



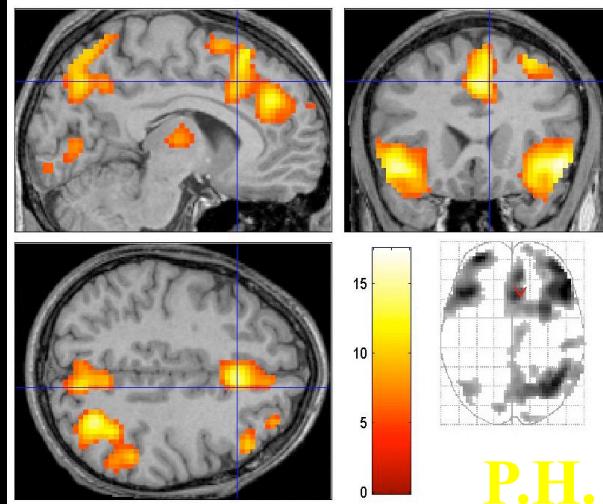
Subject SC 6 months later

Individual patterns of activity are much more consistent across subjects for other retrieval tasks.

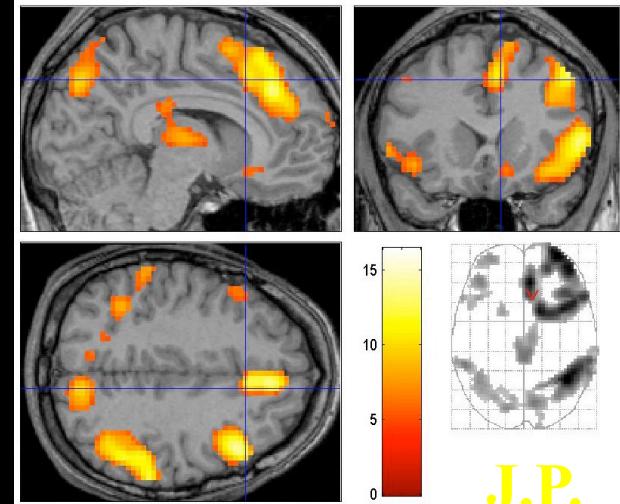
spatial working memory



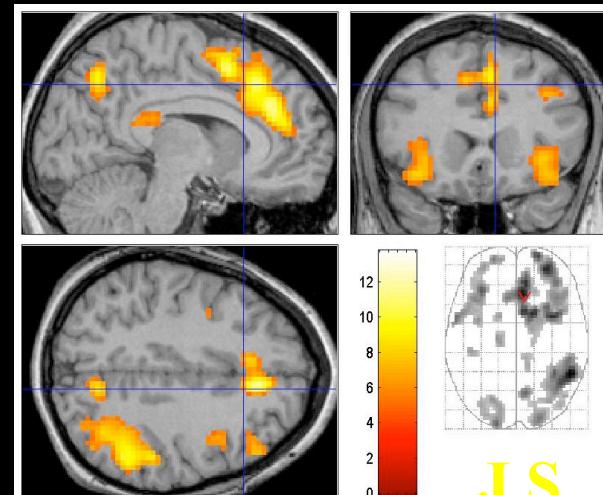
group



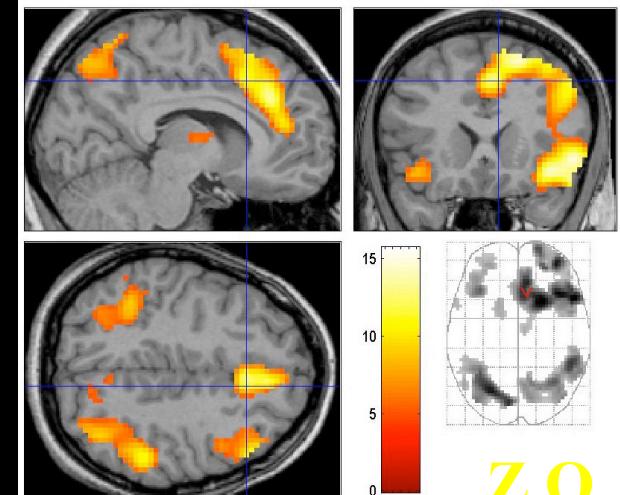
P.H.



J.P.



J.S.



Z.O.

Courtesy, Mike Miler, UC
Santa Barbara and Jack Van
Horn, fMRI Data Center,
Dartmouth University

Local Pattern Effect Classification and Mapping

Functional magnetic resonance imaging (fMRI) "brain reading":
detecting and classifying distributed patterns of fMRI activity
in human visual cortex

David D. Cox^{a,b,*} and Robert L. Savoy^{a,b,c}

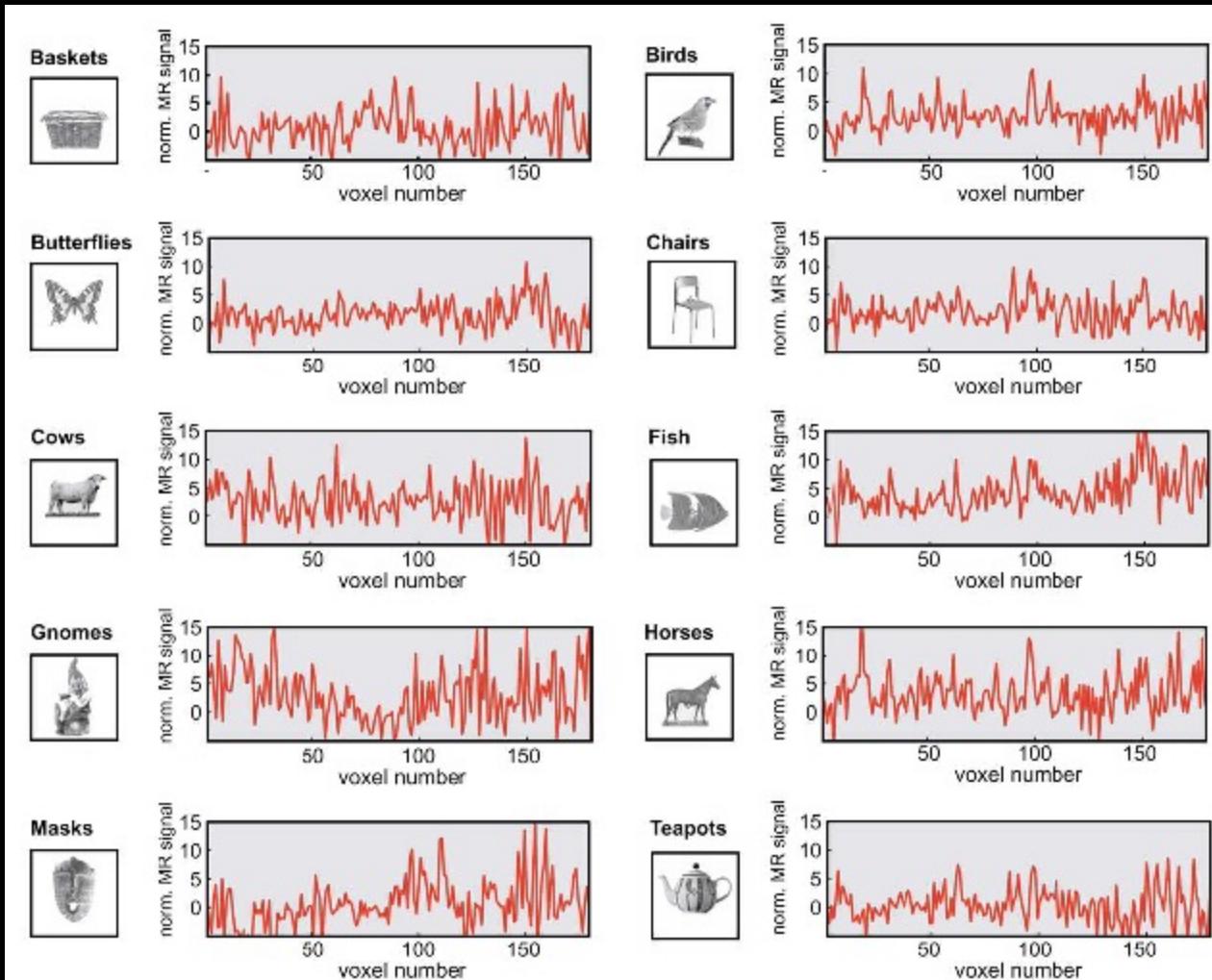
^a Rowland Institute for Science, Cambridge, MA 02142, USA

^b Athinoula A. Martinos Center for Structural and Functional Biomedical Imaging, Charlestown, MA 02129, USA

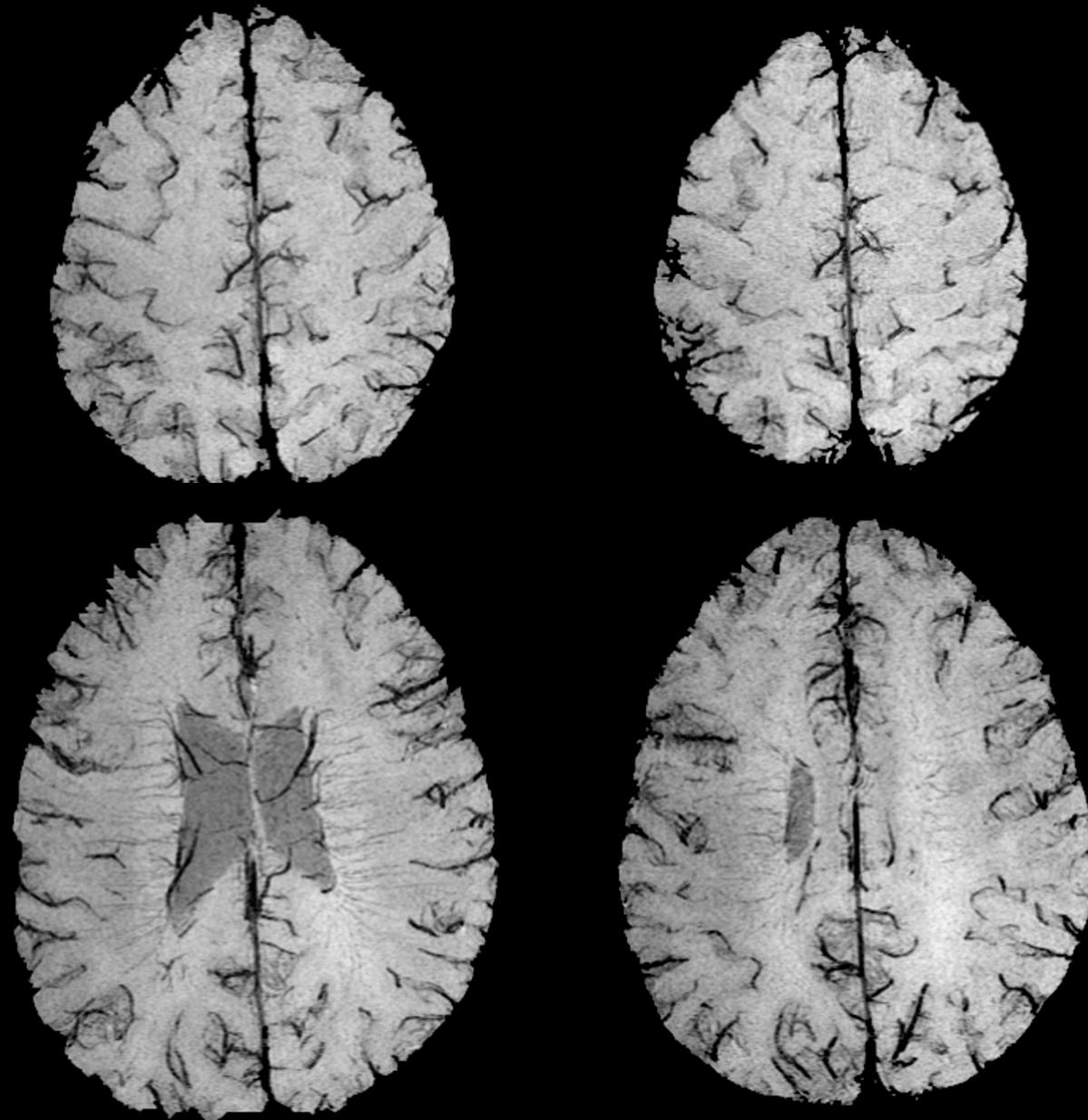
^c HyperVision, Inc., P.O. Box 158, Lexington, MA 02420, USA

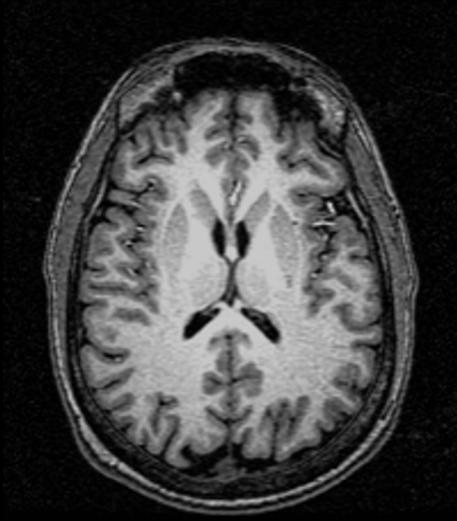
Received 15 July 2002; accepted 10 December 2002

NEUROIMAGE 19 (2): 261-270 Part 1 JUN 2003



Baseline susceptibility mapping

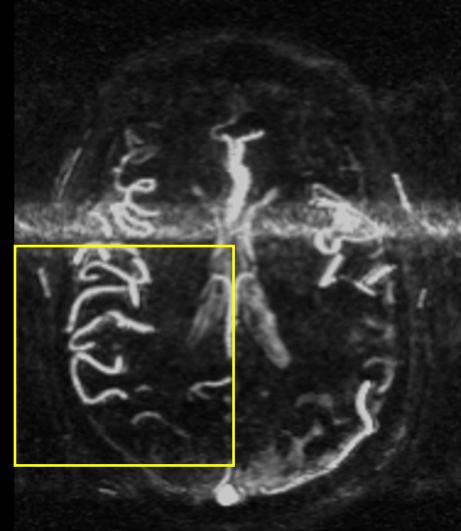




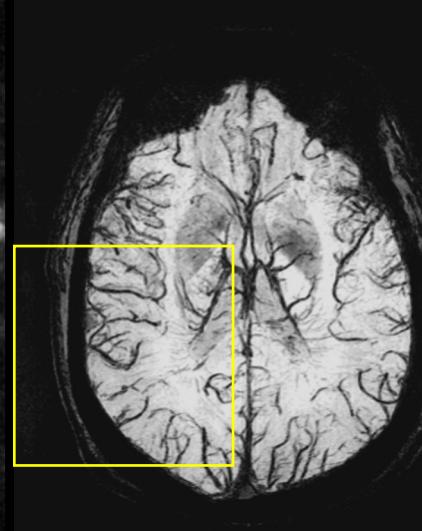
MP-RAGE



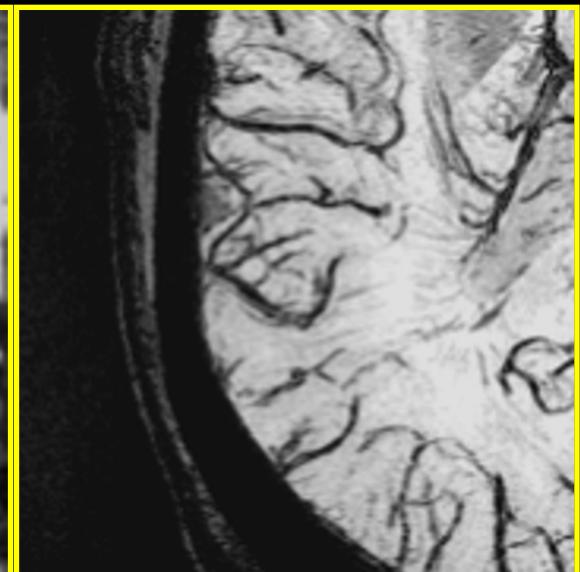
3D T-O-F MRA

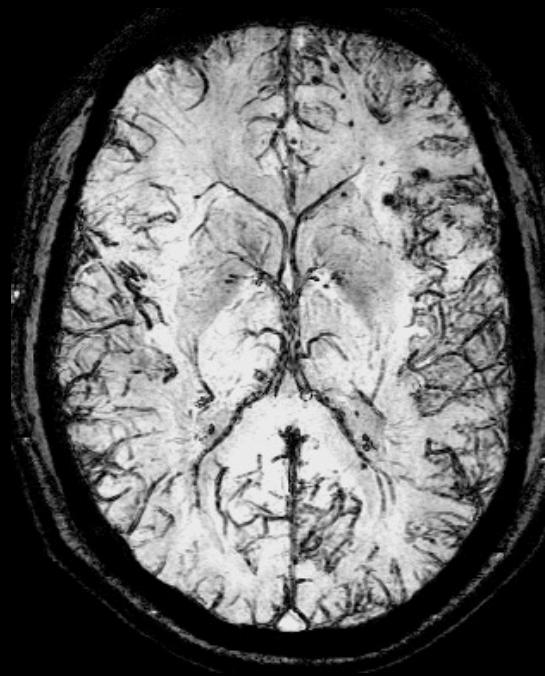
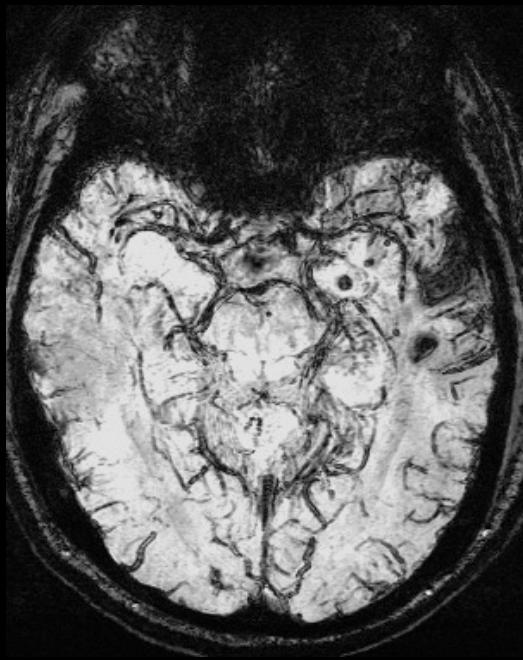


3D Venous PC



MR Venogram



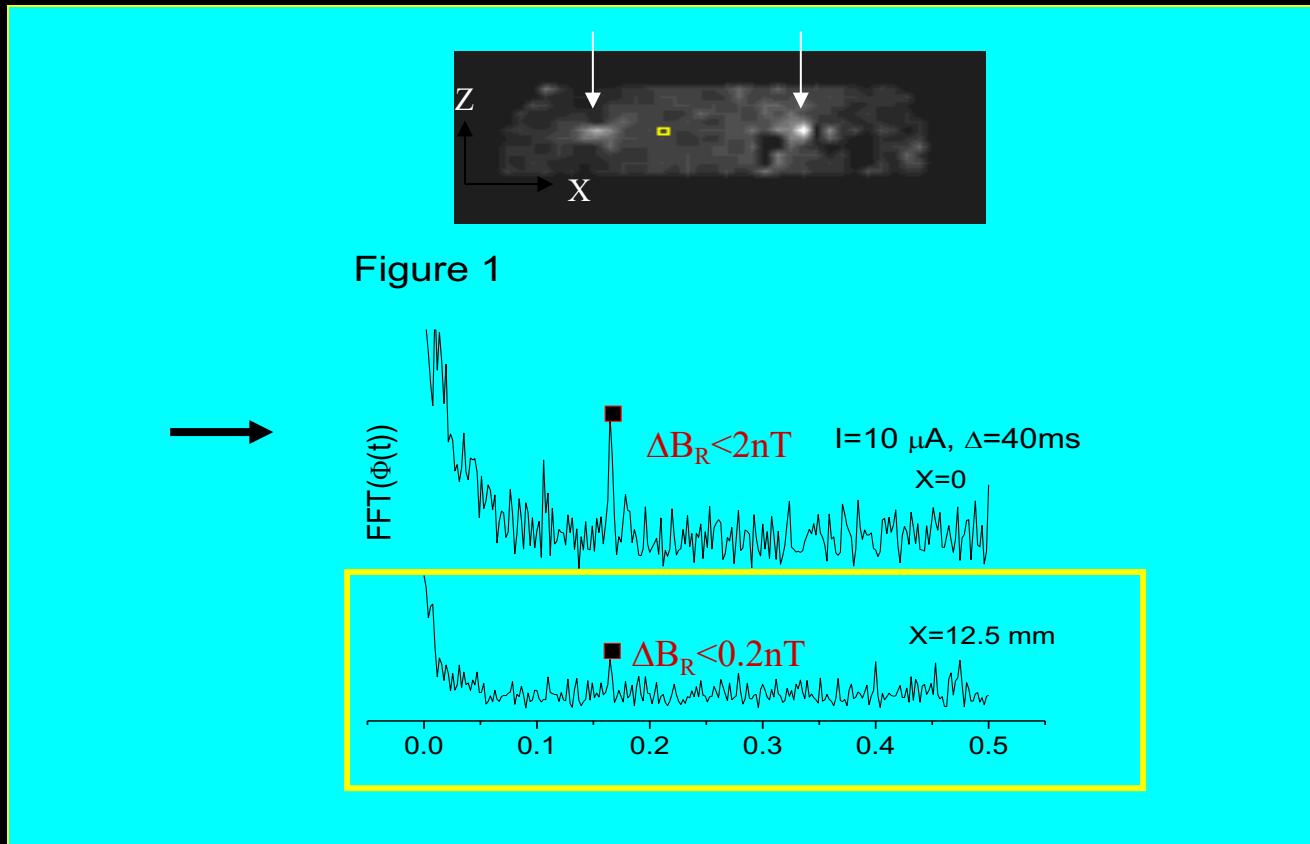
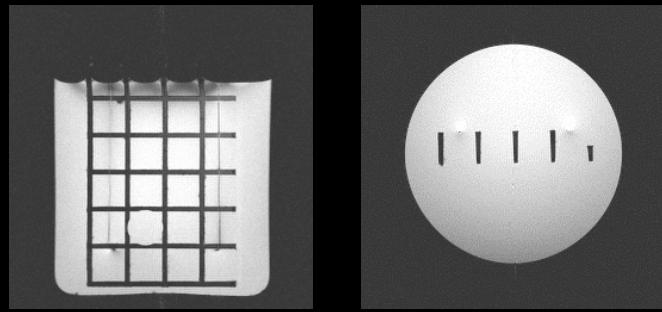


Direct Neuronal Current Imaging?

Toward Direct Mapping of Neuronal Activity: MRI Detection of Ultraweak, Transient Magnetic Field Changes

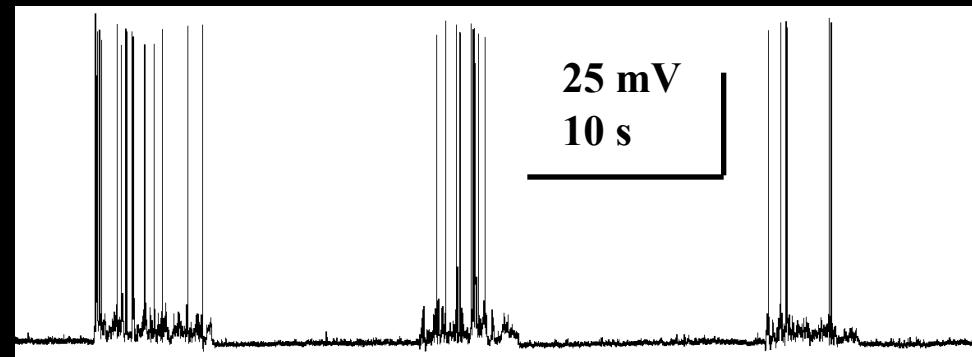
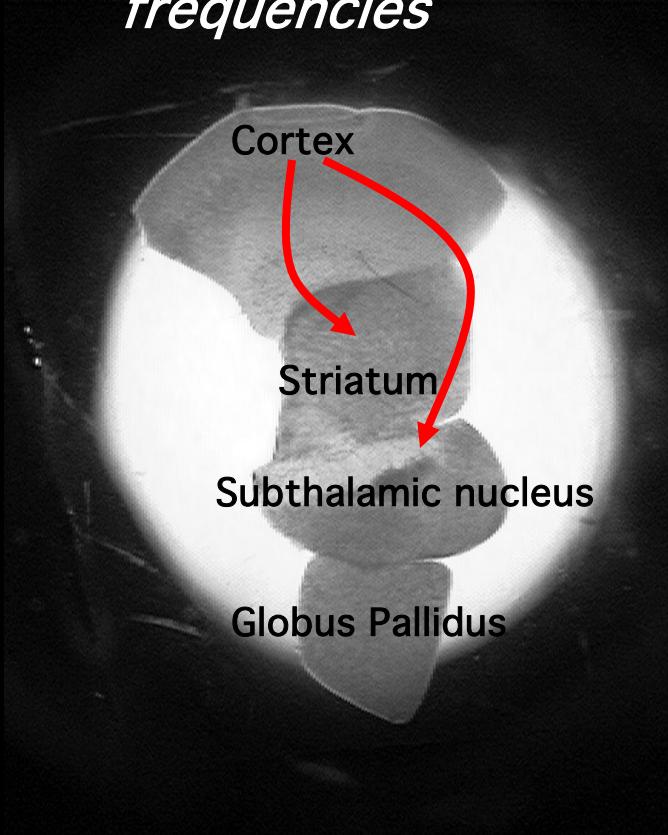
Jerzy Bodurka^{1*} and Peter A. Bandettini^{1,2}

- Preliminary models suggest that magnetic field changes on the order of 0.1 to 1 nT are induced (at the voxel scale) in the brain.
- These changes induce about a 0.01 Hz frequency shift or 0.09 deg (@ TE = 30 ms) phase shift.
- Question: Is this detectable?

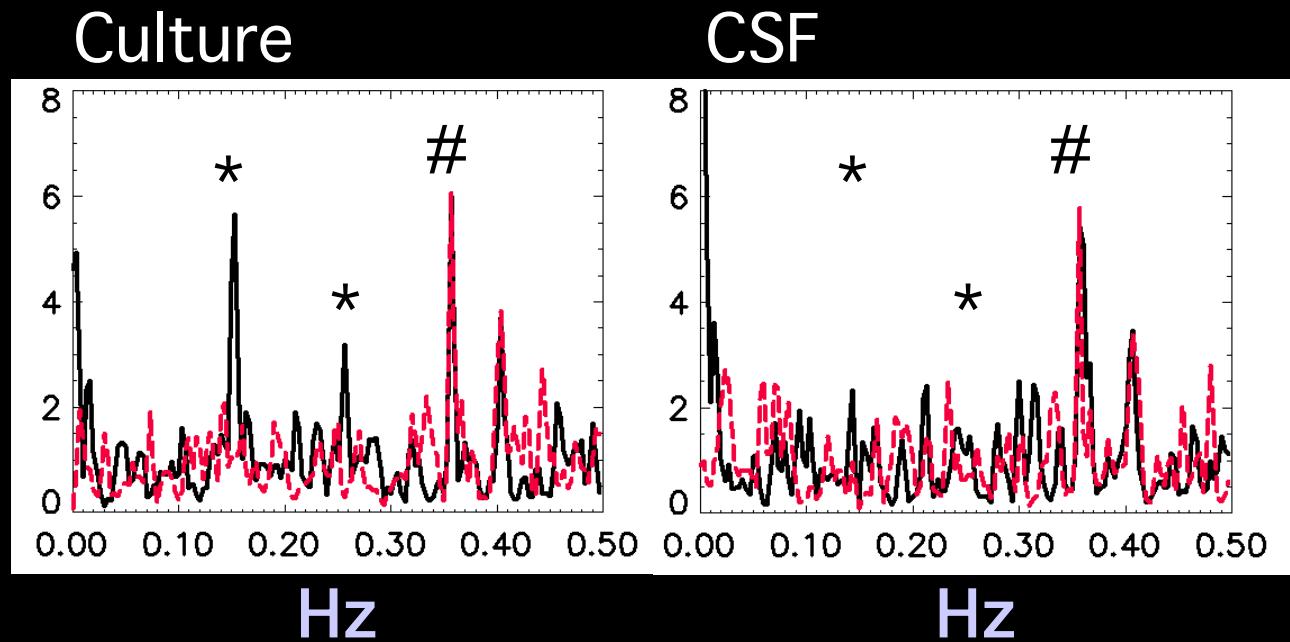
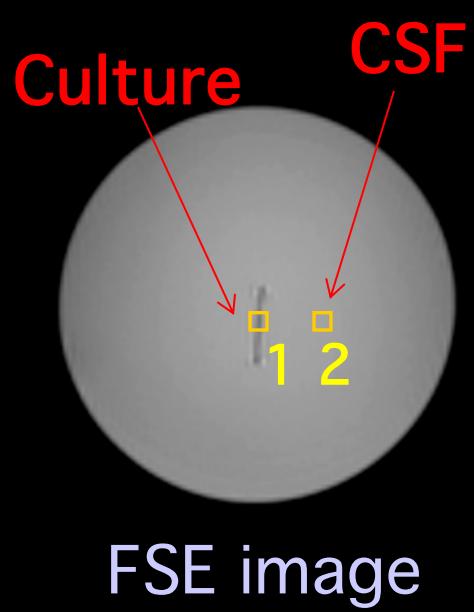


In Vitro Results

Newborn rat brains have been found to exhibit spontaneous and synchronous firing at specific frequencies



Results



Active state: 10 min, Inactive state: 10 min after TTX admin.

*: activity

#: scanner pump frequency

What are the biggest unknowns/challenges?

1. Technology
2. Methodology
3. Interpretation

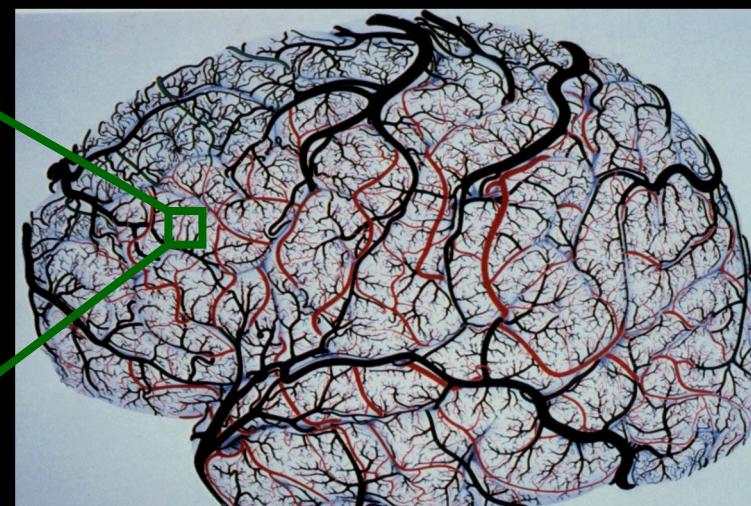
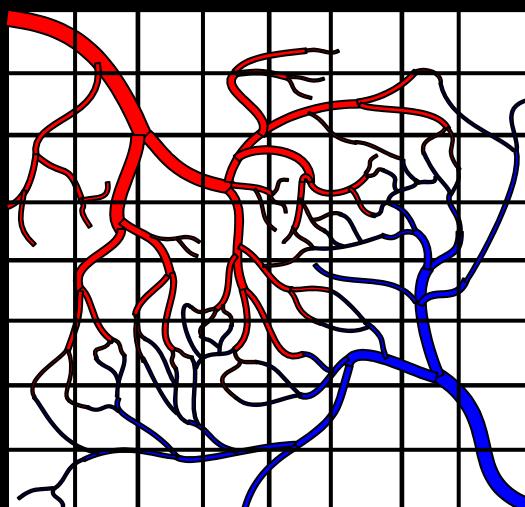
Interpretation

- Linearity / proportionality
- Hemodynamic vs. Neuronal effects
- Resting state (fluctuations and DC)
- Neuronal inhibition / excitation effects
- Negative signal changes
- HRF latency, magnitude, pre and post undershoot
- T2, T2*, T1, diffusion, and Mo changes
- Differences across modalities (location, timing)

Interpretation

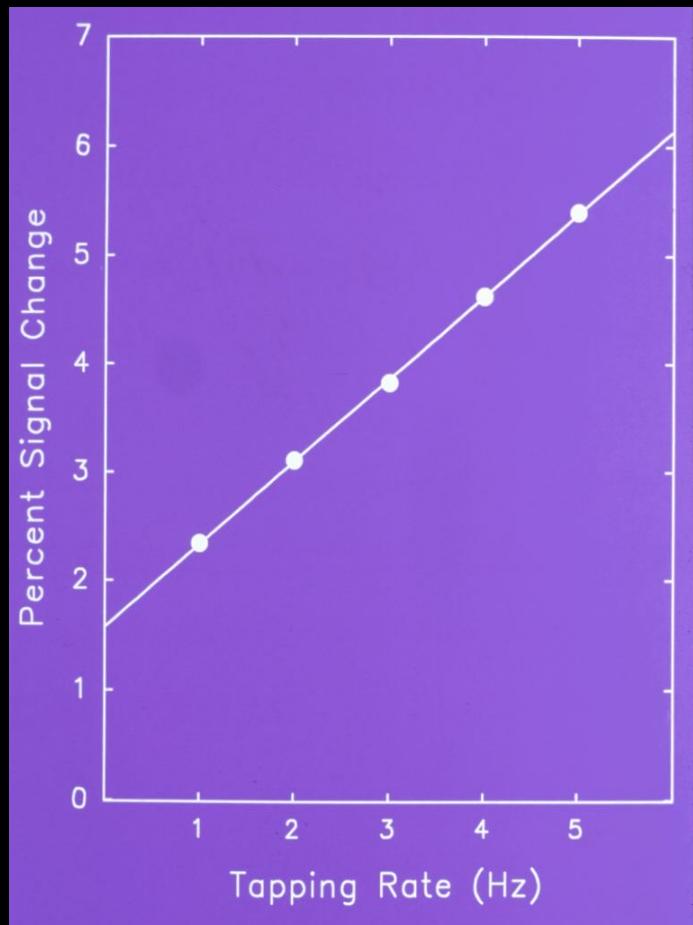
- Linearity / proportionality
- Hemodynamic vs. Neuronal effects
- Resting state (fluctuations and DC)
- Neuronal inhibition / excitation effects
- Negative signal changes
- HRF latency, magnitude, pre and post undershoot
- T2, T2*, T1, diffusion, and Mo changes
- Differences across modalities (location, timing)

The Problem

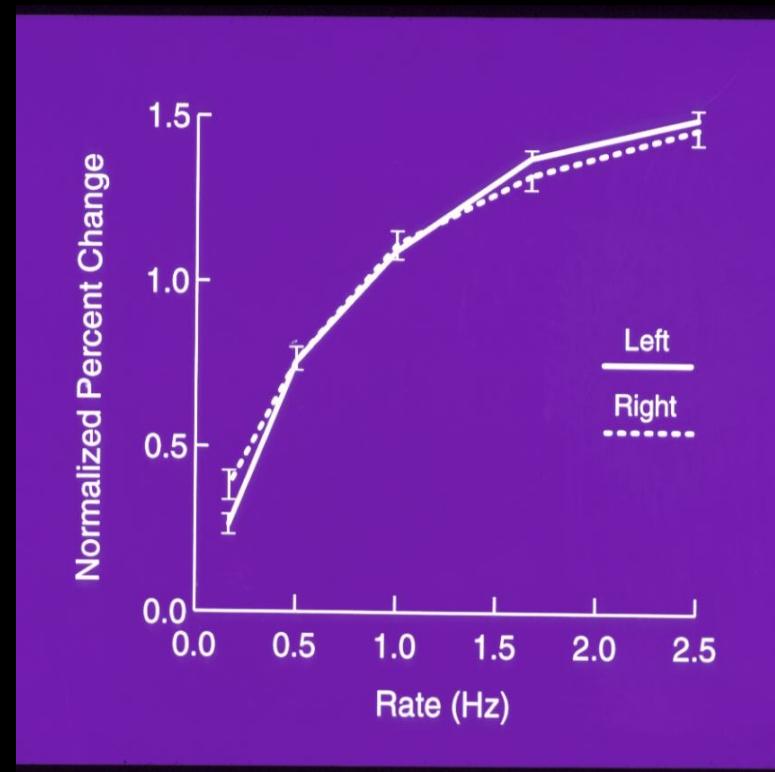


Linearity / proportionality

Motor Cortex



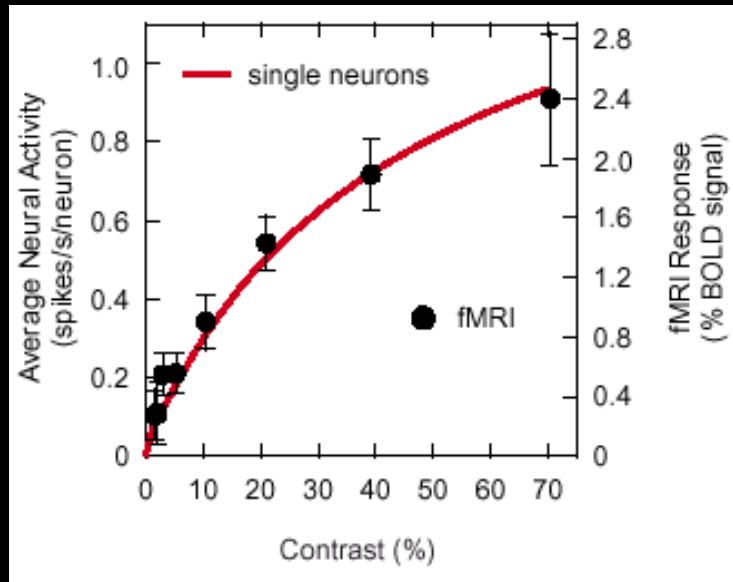
Auditory Cortex



S. M. Rao et al, (1996) "Relationship between finger movement rate and functional magnetic resonance signal change in human primary motor cortex." *J. Cereb. Blood Flow and Met.* 16, 1250-1254.

J. R. Binder, et al, (1994). "Effects of stimulus rate on signal response during functional magnetic resonance imaging of auditory cortex." *Cogn. Brain Res.* 2, 31-38

fMRI responses in human V1 are proportional to average firing rates in monkey V1



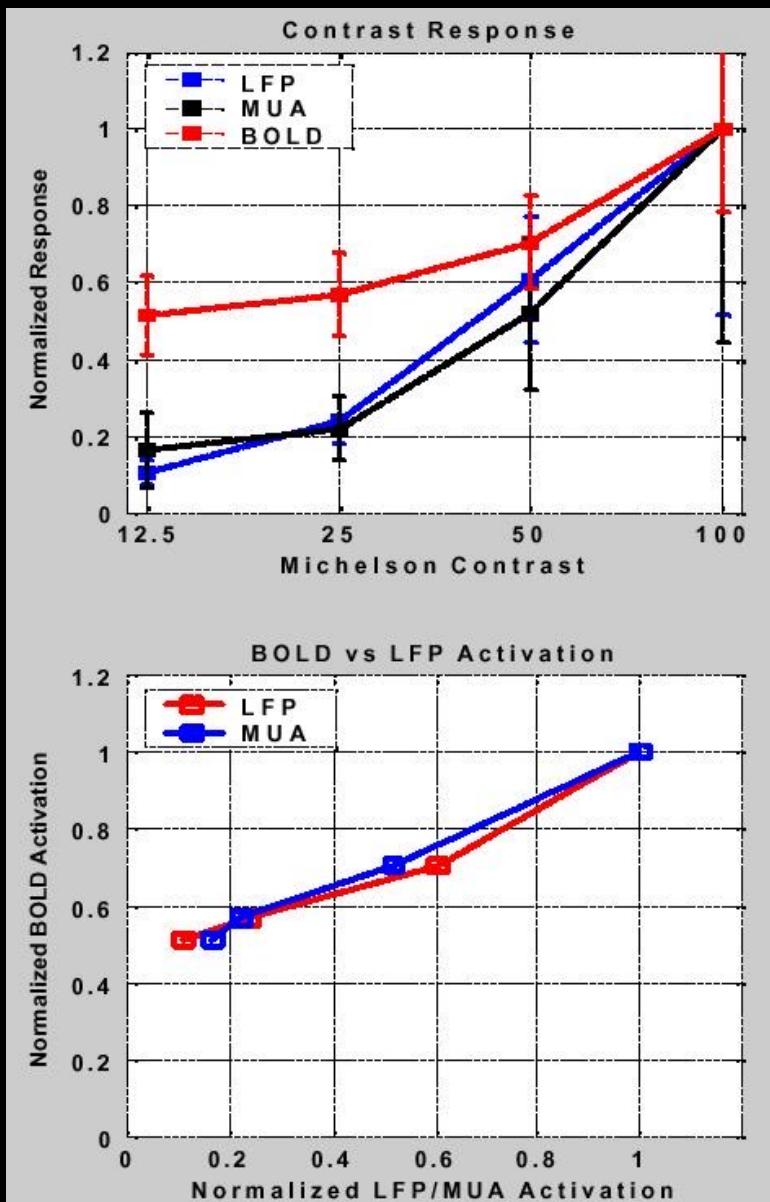
Heeger, D. J., Huk, A. C., Geisler, W. S., and Albrecht, D. G. 2000. Spikes versus BOLD: What does neuroimaging tell us about neuronal activity? *Nat. Neurosci.* 3: 631–633.

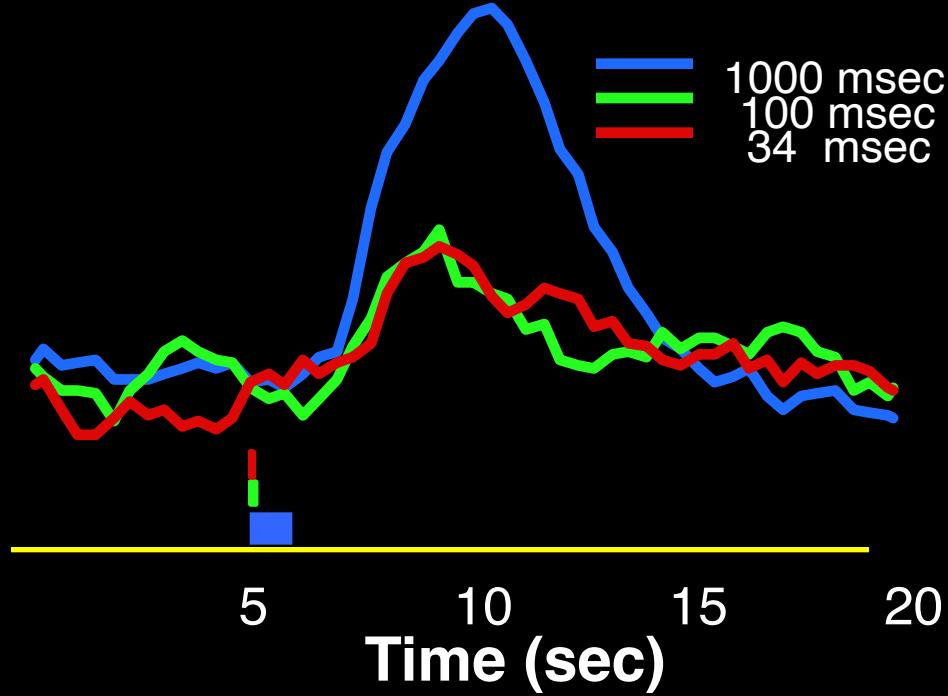
0.4 spikes/sec -> 1% BOLD

Rees, G., Friston, K., and Koch, C. 2000. A direct quantitative relationship between the functional properties of human and macaque V5. *Nat. Neurosci.* 3: 716–723.

9 spikes/sec -> 1% BOLD

Logothetis et al. (2001) "Neurophysiological investigation of the basis of the fMRI signal" Nature, 412, 150-157

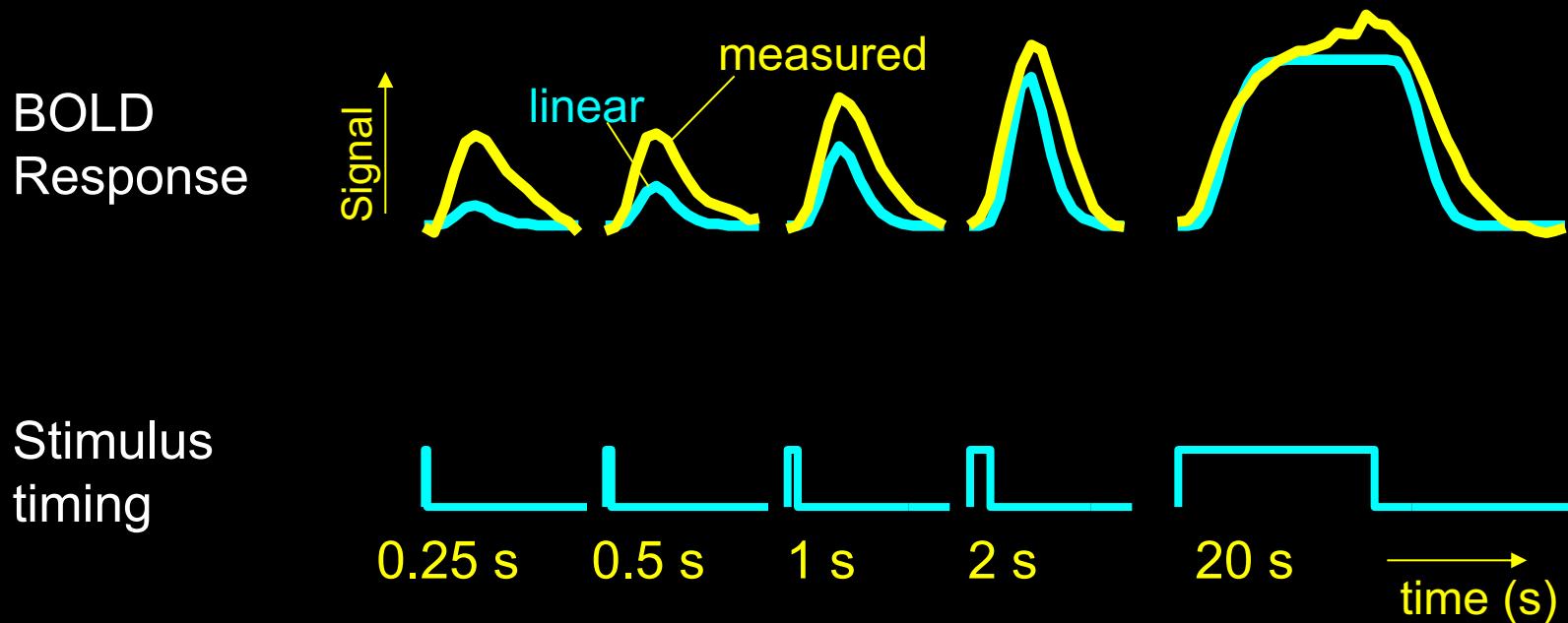




R. L. Savoy, et al., Pushing the temporal resolution of fMRI: studies of very brief visual stimuli, onset variability and asynchrony, and stimulus-correlated changes in noise [oral], 3'rd Proc. Soc. Magn. Reson., Nice, p. 450. (1995).

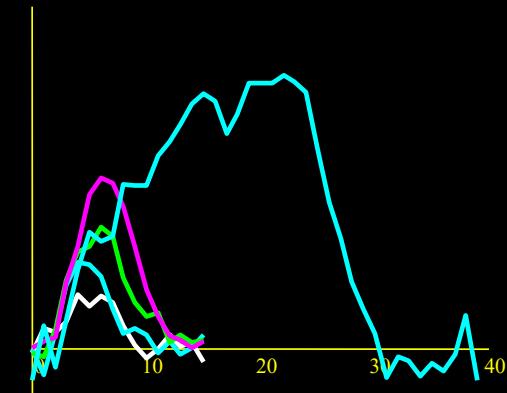
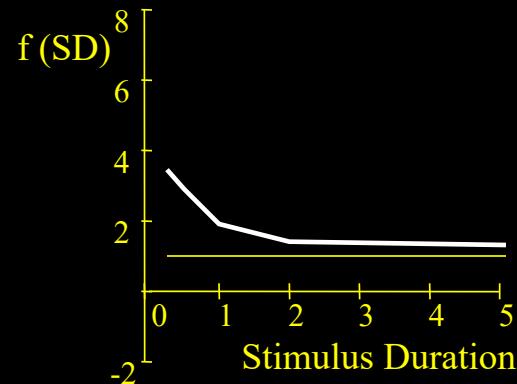
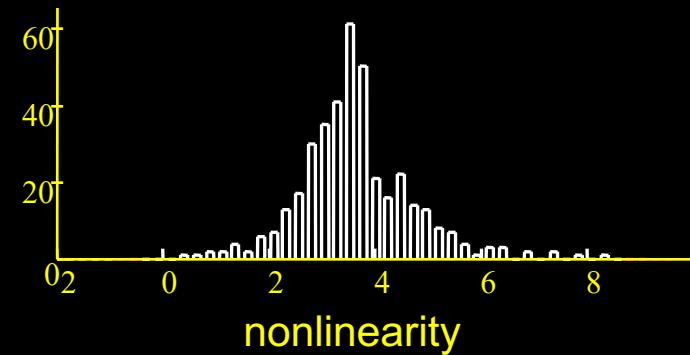
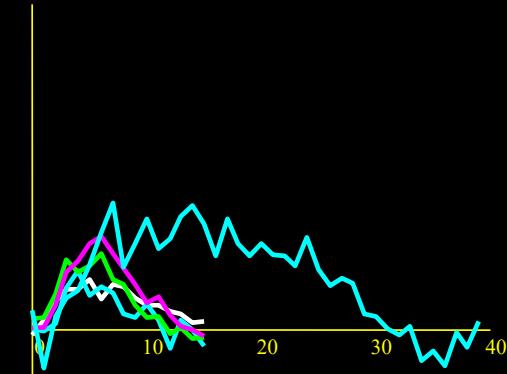
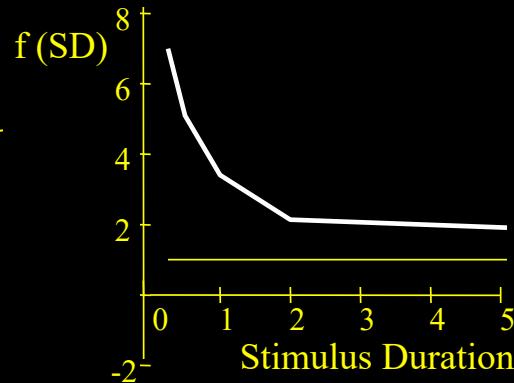
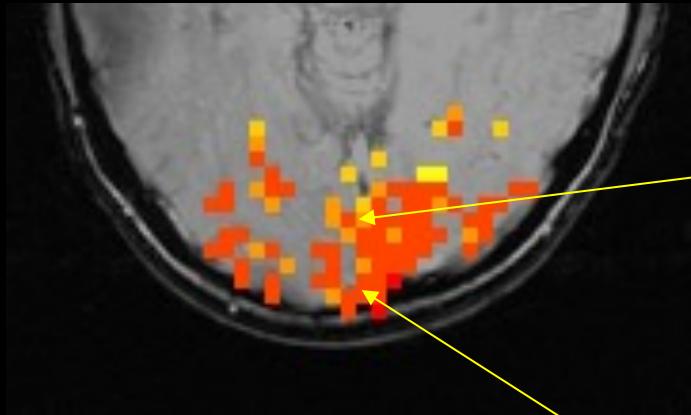
Dynamic Nonlinearity Assessment

Different stimulus “ON” periods



Brief stimuli produce larger responses than expected

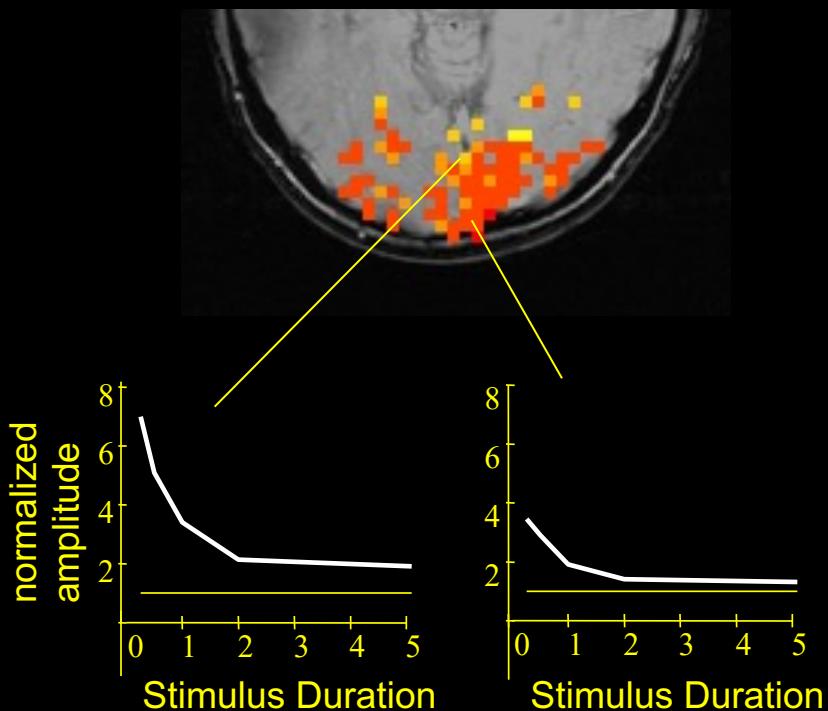
Spatial Heterogeneity of BOLD Nonlinearity



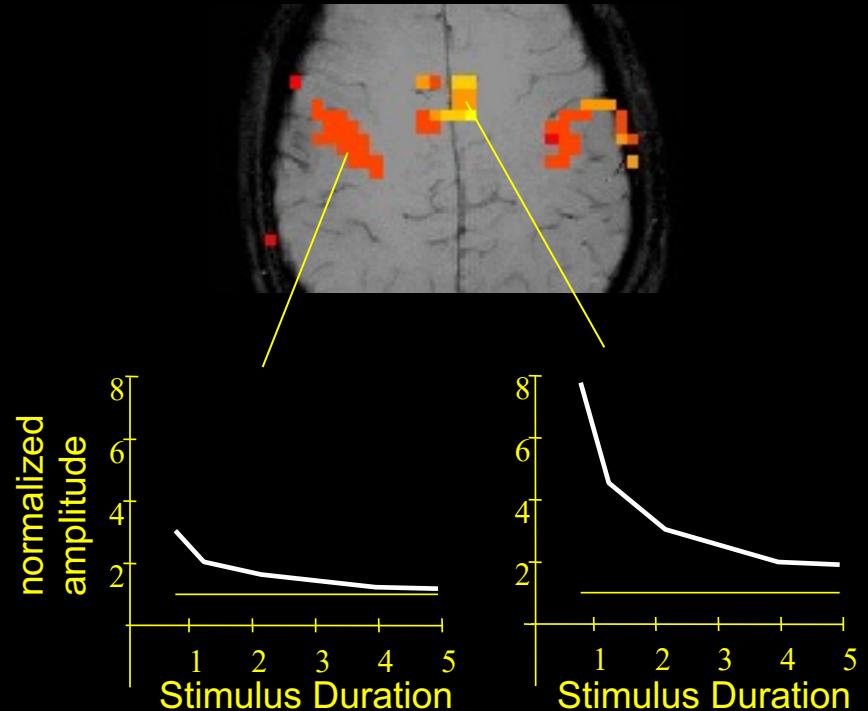
R. M. Birn, Z. Saad, P. A. Bandettini, (2001) “Spatial heterogeneity of the nonlinear dynamics in the fMRI BOLD response.” *NeuroImage*, 14: 817-826.

Spatial variation of linearity

Visual

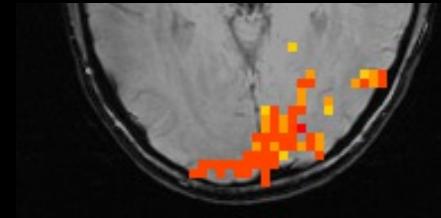
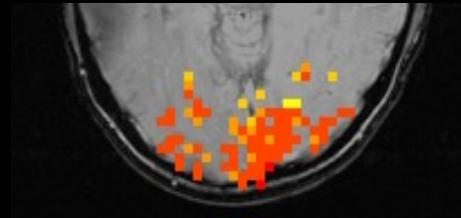
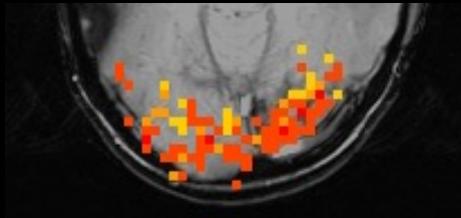


Motor

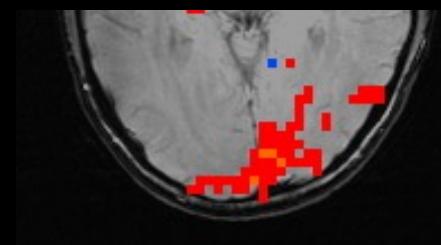
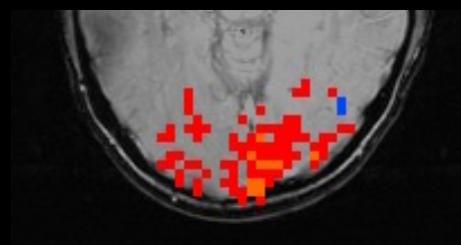
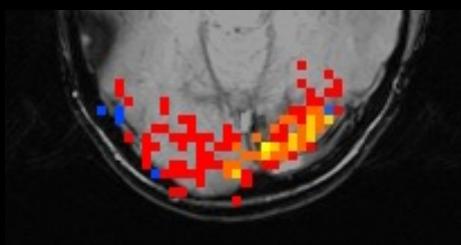


Results – visual task

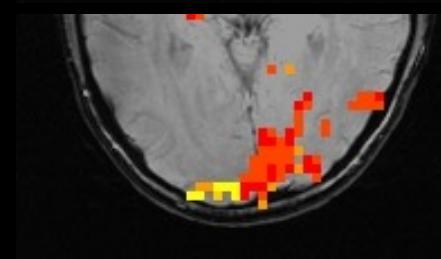
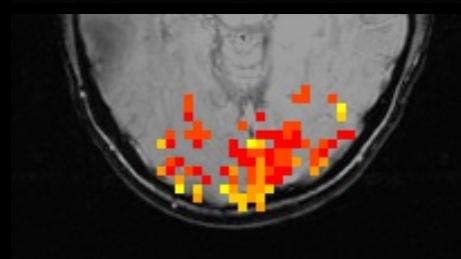
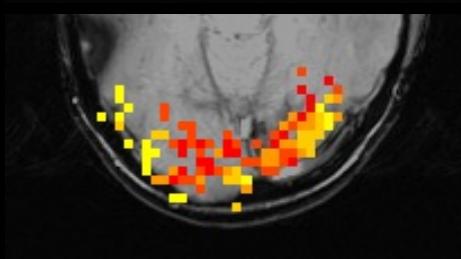
Nonlinearity



Magnitude

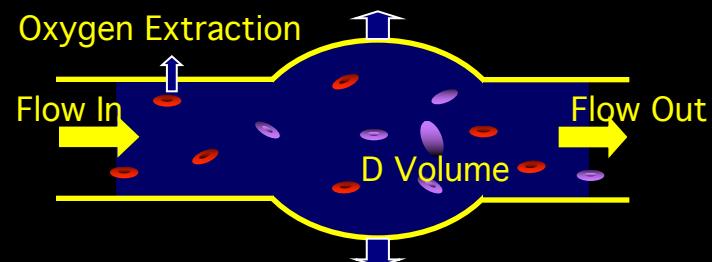
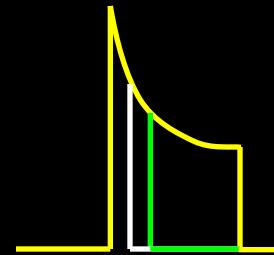


Latency



Sources of this Nonlinearity

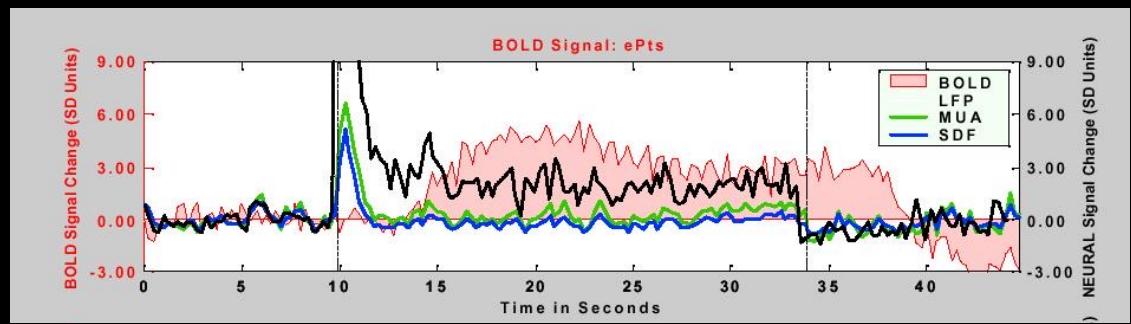
- Neuronal
- Hemodynamic
 - Oxygen extraction
 - Blood volume dynamics



BOLD Correlation with Neuronal Activity

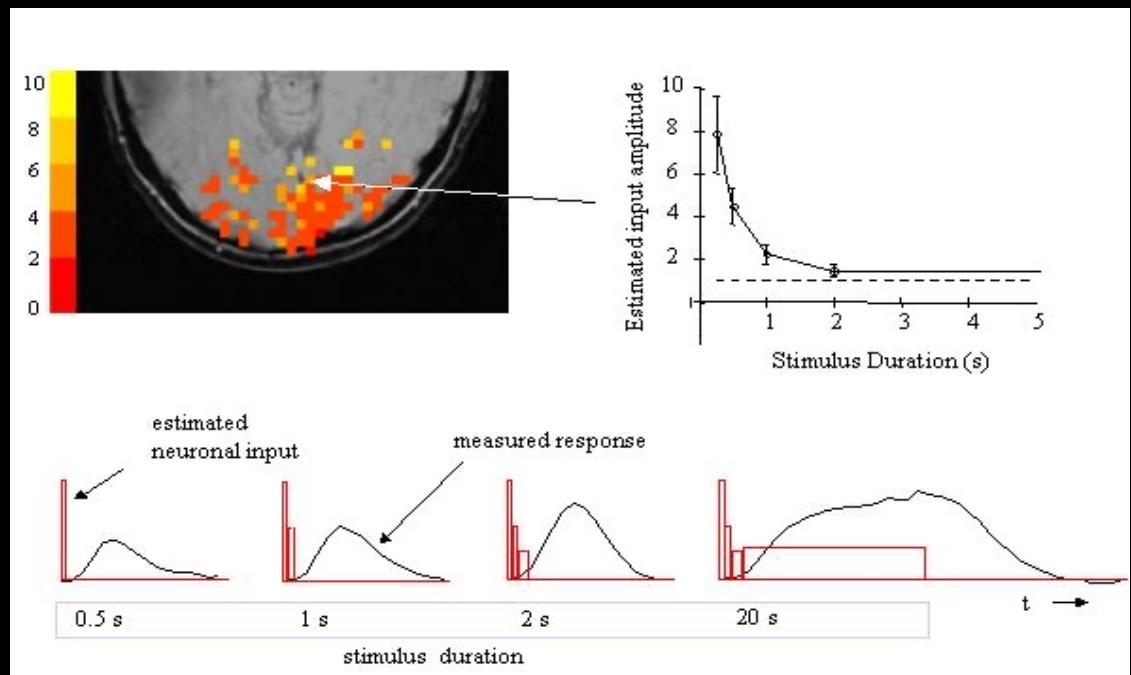
Logothetis et al. (2001)

“Neurophysiological investigation
of the basis of the fMRI signal”
Nature, 412, 150-157.



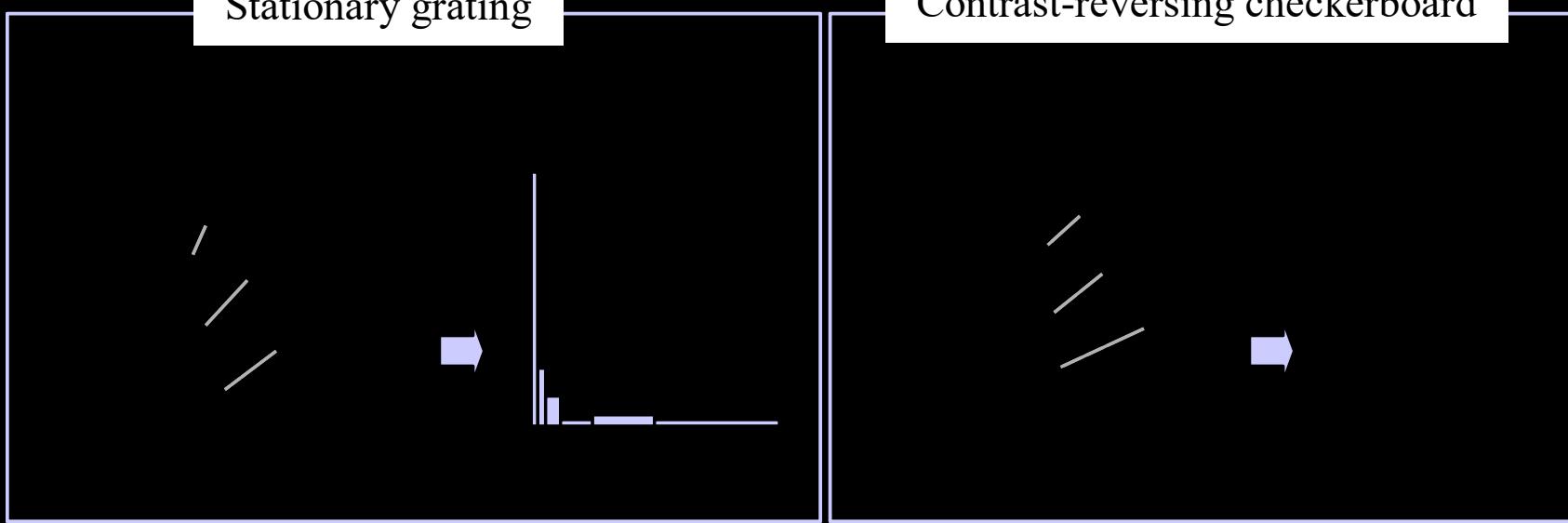
P. A. Bandettini and L. G.

Ungerleider, (2001) “From neuron
to BOLD: new connections.”
Nature Neuroscience, 4: 864-866.



Stationary grating

Contrast-reversing checkerboard



Acknowledgements: FIM and FMRI

Director:

Peter Bandettini

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Sean Marrett

Jerzy Bodurka

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Wen-Ming Luh

Rasmus Birn

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Adam Thomas

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