

# Latest Developments in fMRI

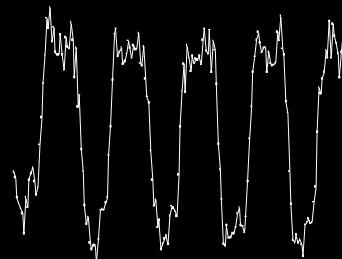
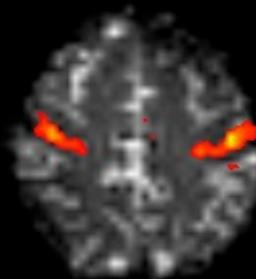
Peter A. Bandettini, Ph.D

Unit on Functional Imaging Methods  
&  
3T Neuroimaging Core Facility

Laboratory of Brain and Cognition  
National Institute of Mental Health

# The use of fMRI for the Investigation of Brain Function and Physiology

- Where?



- When?

- How much?

- How to get the brain to do what we want it to do in the context of an fMRI experiment?

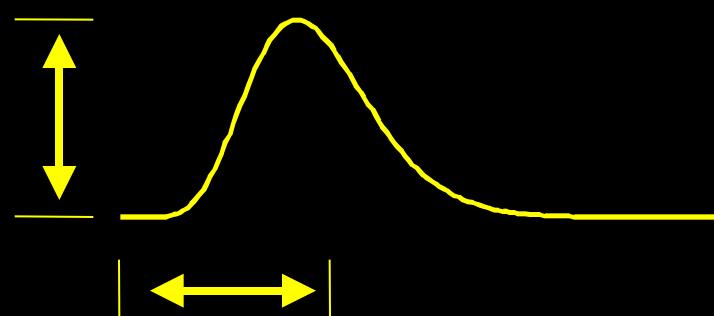
*(limitations: limited time and signal to noise, motion, acoustic noise)*

- How much more information can we obtain?

**Neuronal  
Activation**

**Measured  
fMRI  
Signal**

**Hemodynamics**



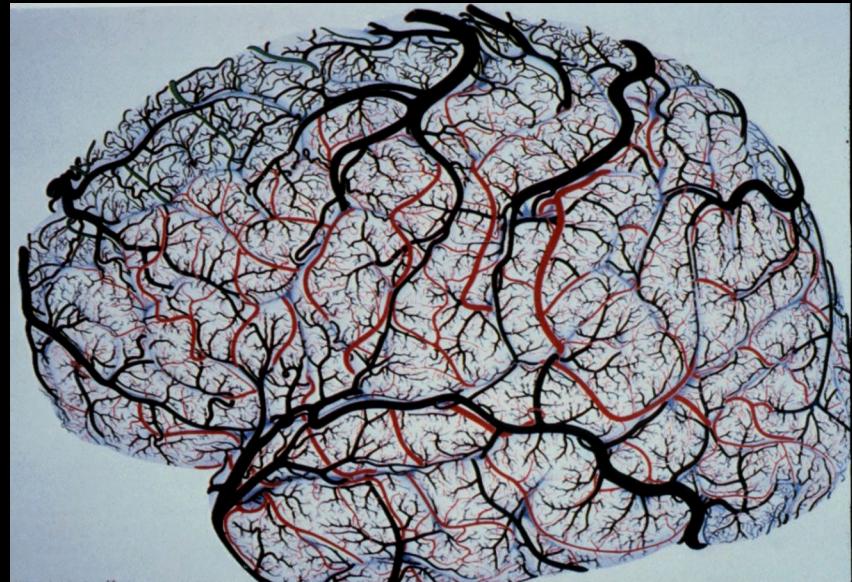
**Physiologic Factors**

# A Primary Challenge for Observing Brain Activation:

...to make progressively more precise inferences without making too many assumptions about non-neuronal physiologic factors.



FIG. 43. Middle temporal gyrus. Female, 60 years. (1) Principal intracortical vein. The branches length regularly decreases from deep towards superficial cortical regions, thus the vascular territory of the principal vein has a conical appearance (dotted line) ( $\times 28$ ).

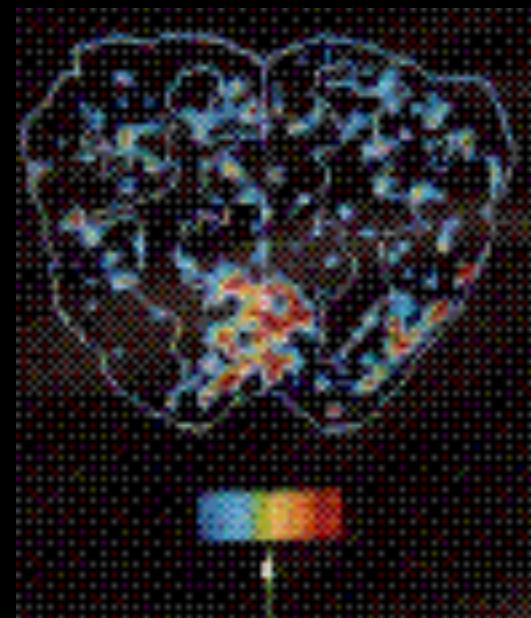
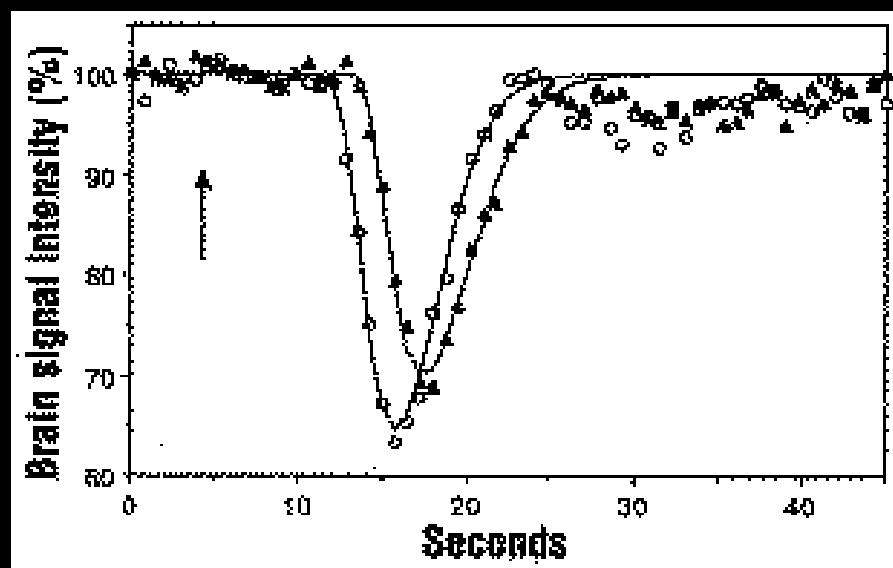
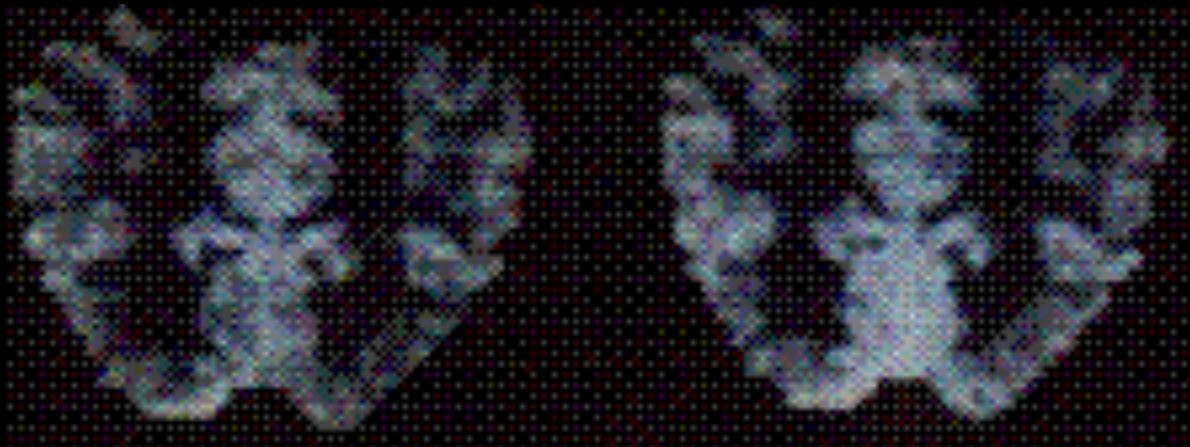


# Contrast in Functional MRI

- **Blood Volume**
  - Contrast agent injection and time series collection of T2\* or T2 - weighted images
- **BOLD**
  - Time series collection of T2\* or T2 - weighted images
- **Perfusion**
  - T1 weighting
  - Arterial spin labeling

**Resting**

**Active**

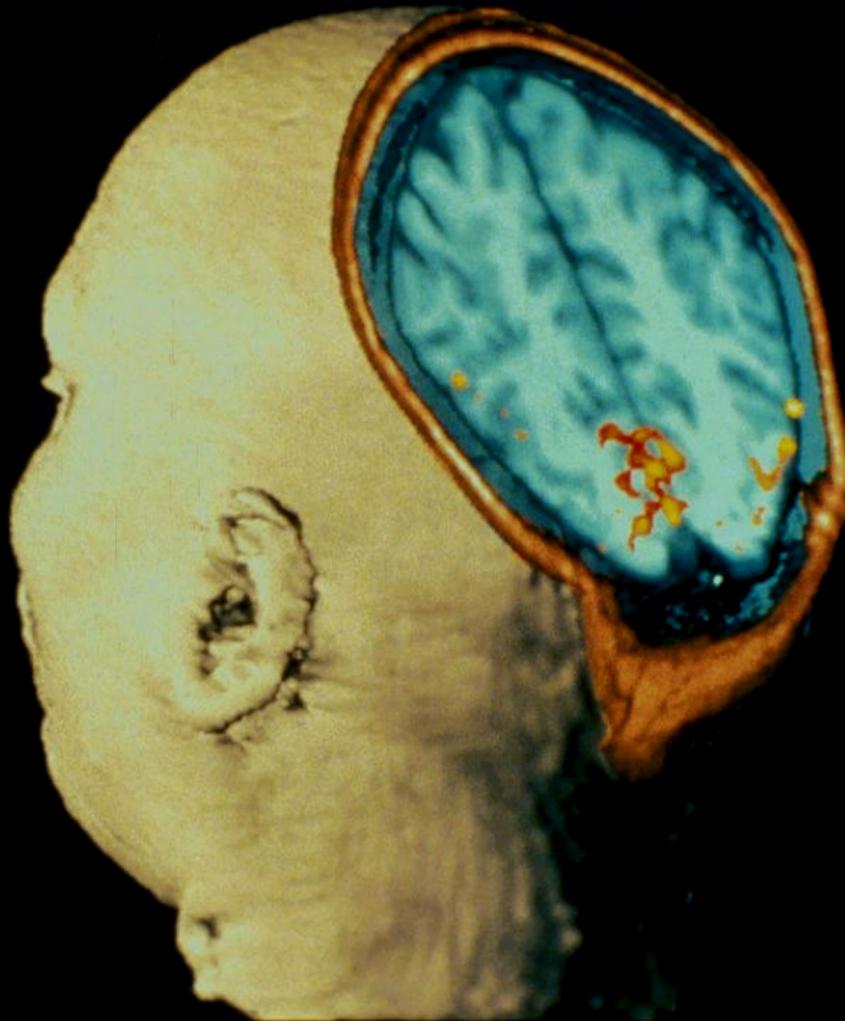


# Photic Stimulation

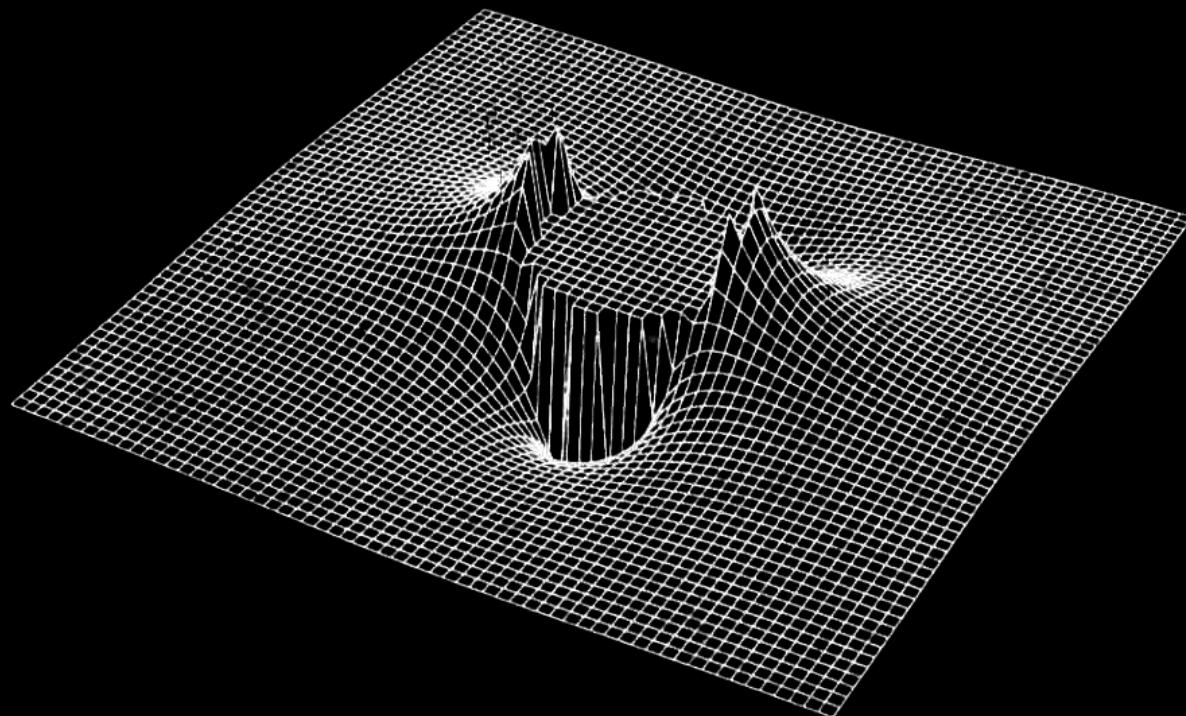
MRI Image showing  
activation of the  
Visual Cortex

From Belliveau, et al.  
Science Nov 1991

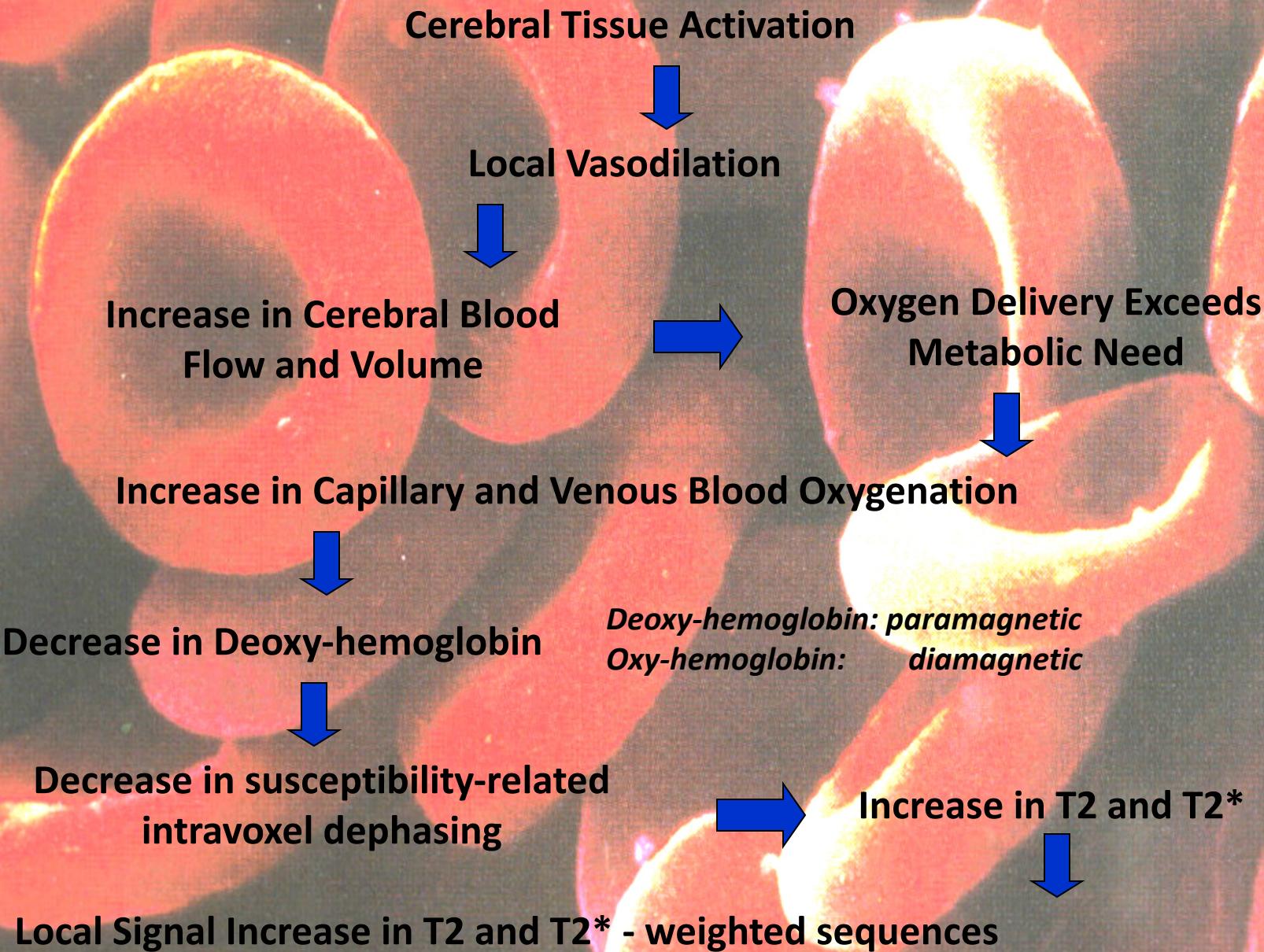
MSC - perfusion



Susceptibility-Induced Field Distortion in the  
Vicinity of a Microvessel  $\perp$  to  $B_0$ .

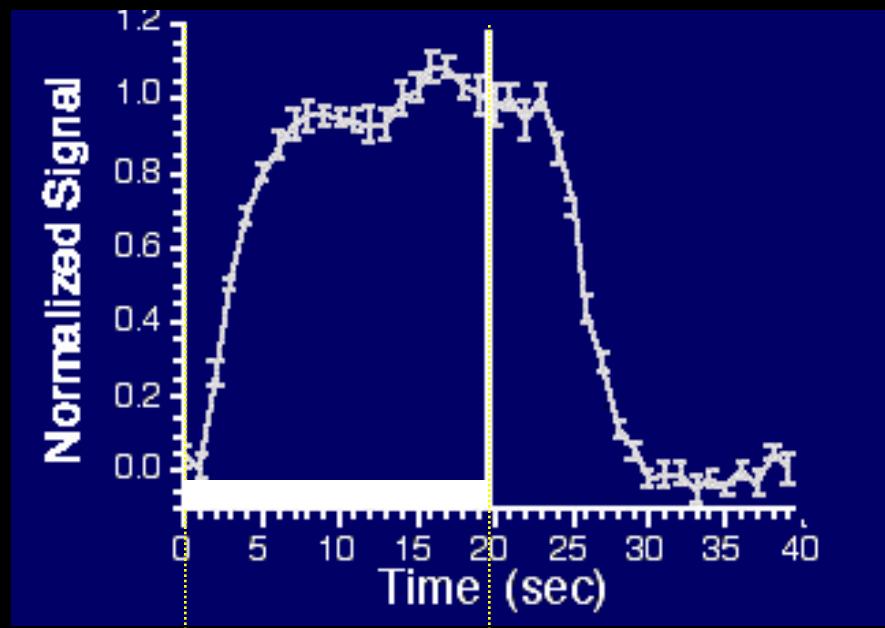


# BOLD Contrast in the Detection of Neuronal Activity

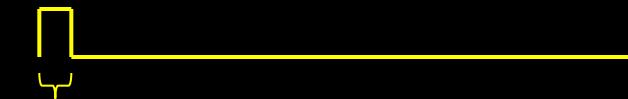
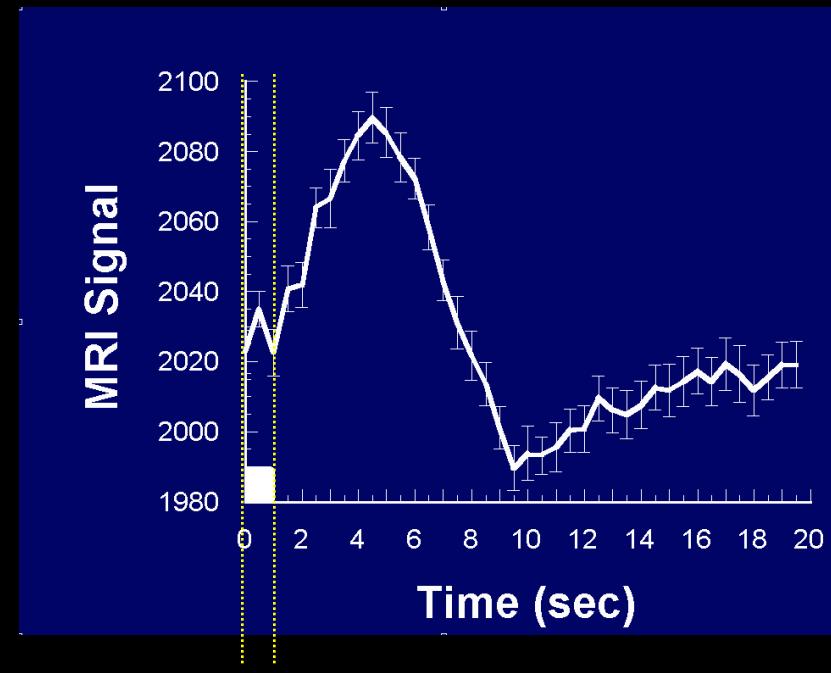


# The BOLD Signal

Blood Oxxygenation Level Dependent (BOLD) signal changes



*task*

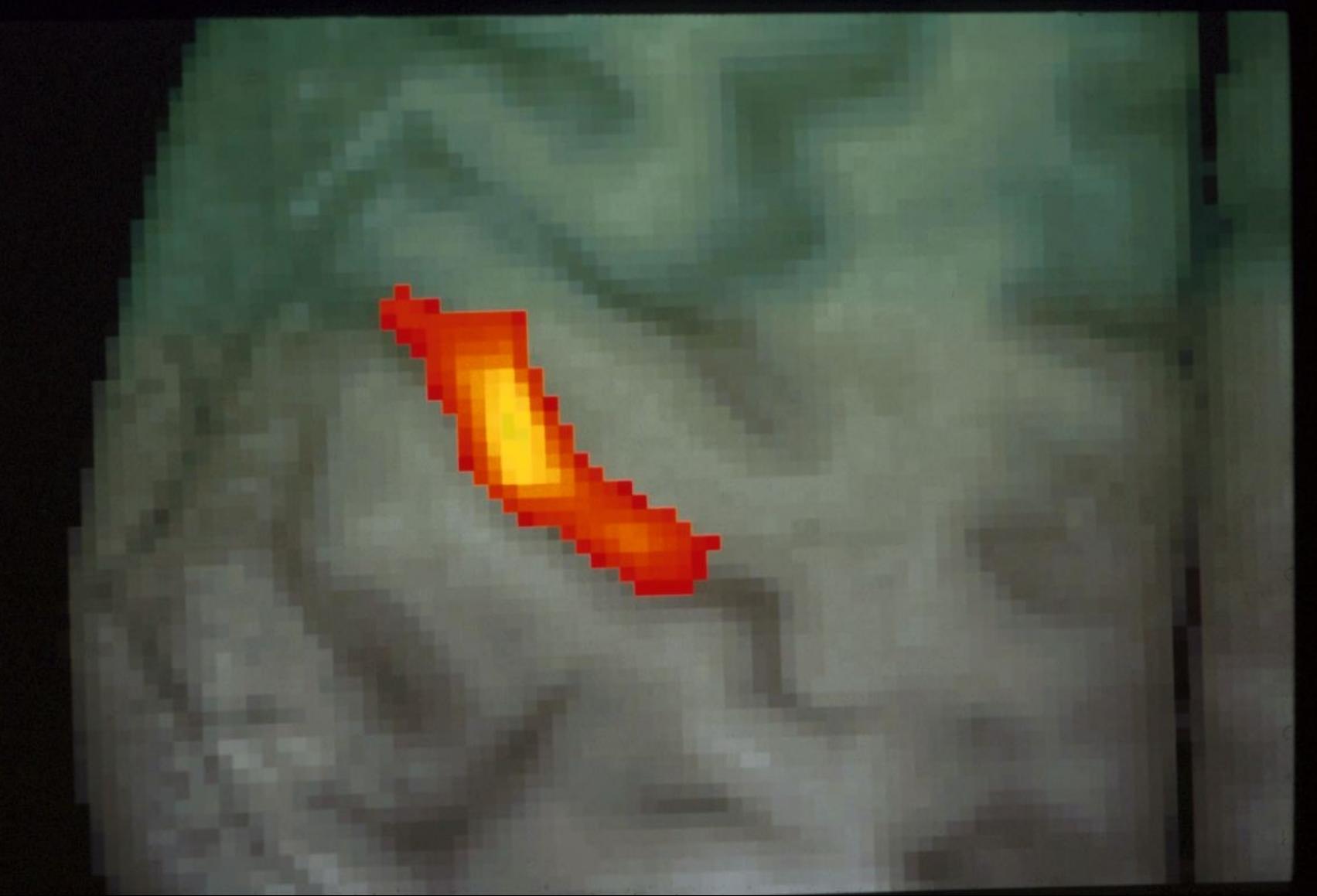


*task*

# Alternating Left and Right Finger Tapping

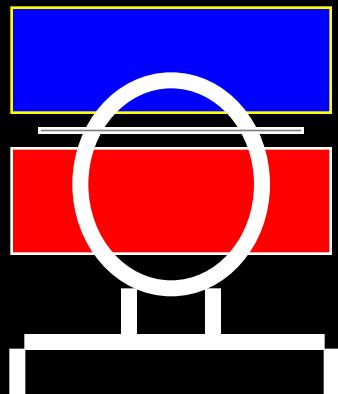


~ 1992

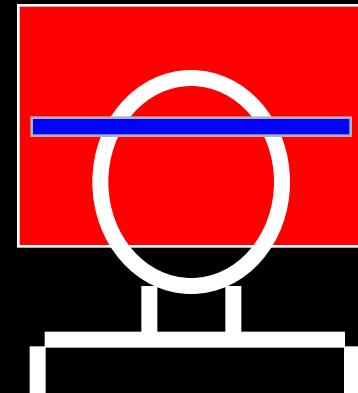


# Perfusion / Flow Imaging

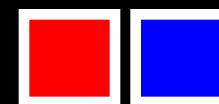
EPISTAR



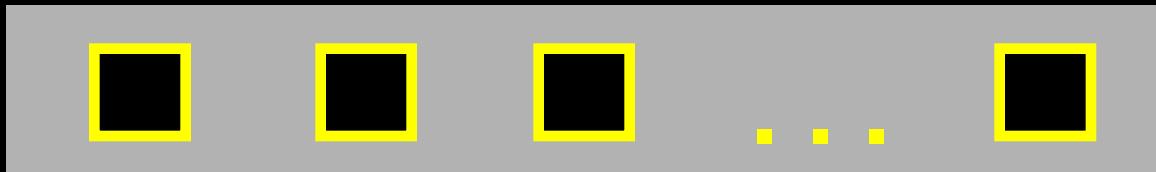
FAIR



...

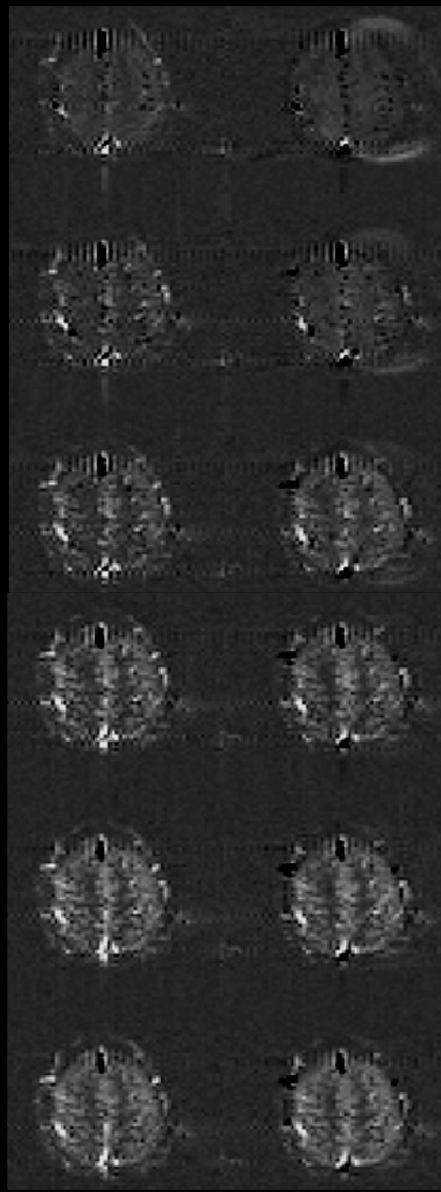


...



**TI (ms) FAIR EPISTAR**

**200**



**400**

**600**

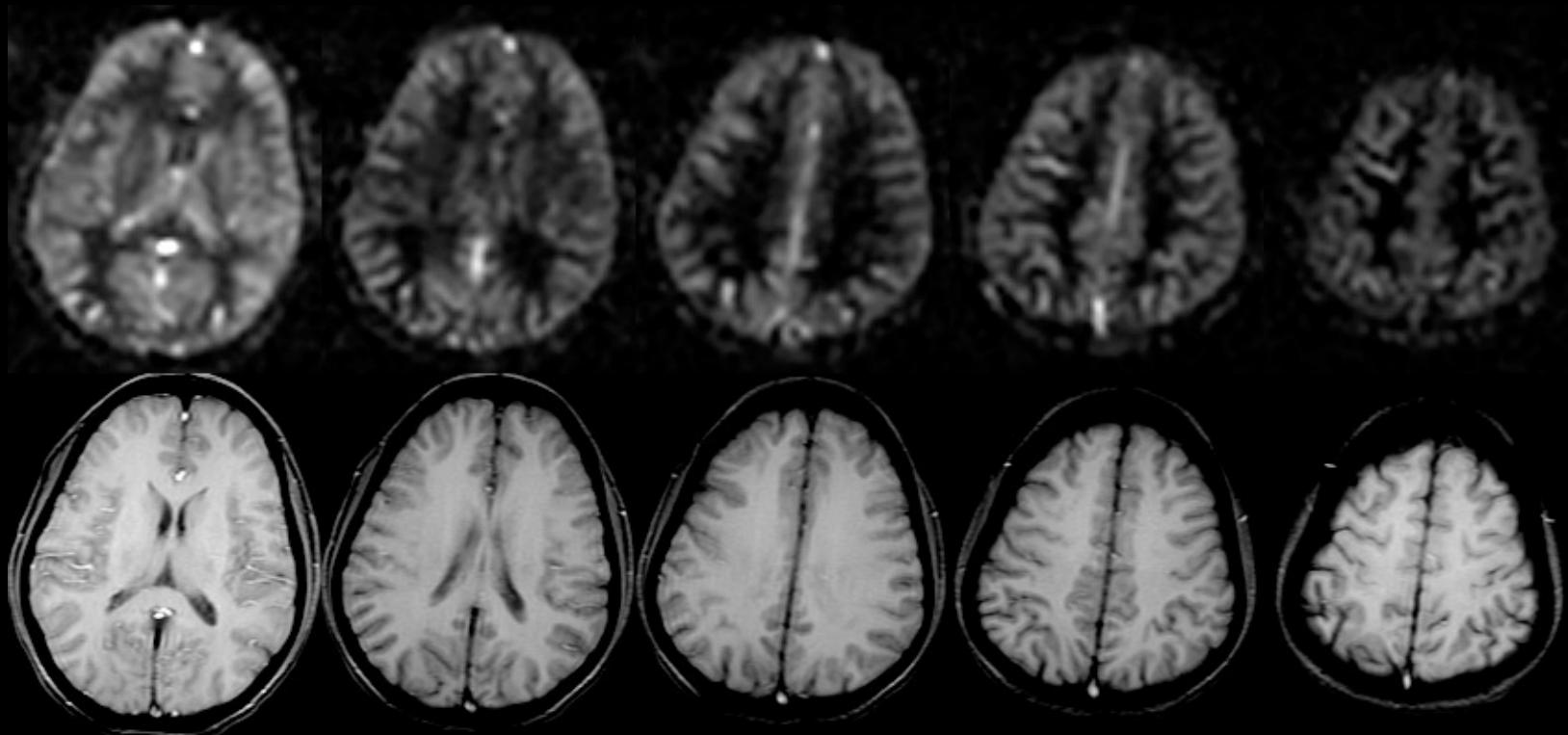
**800**

**1000**

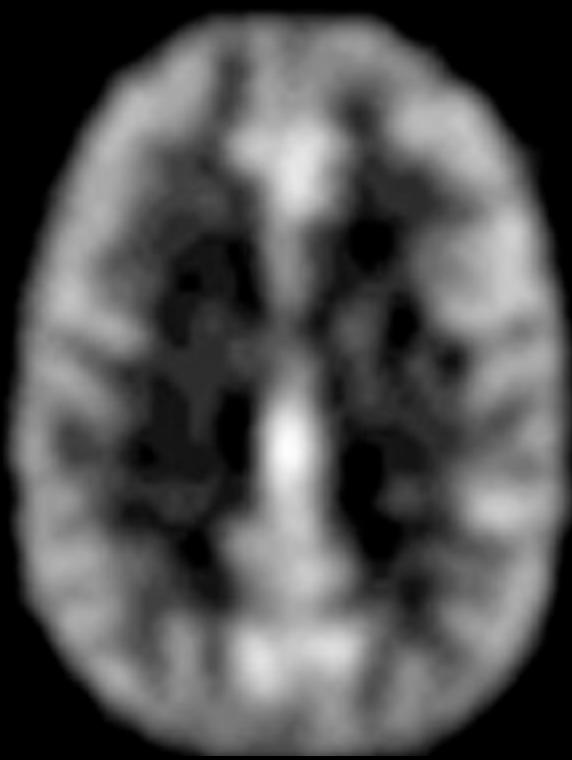
**1200**

# Resting ASL Signal

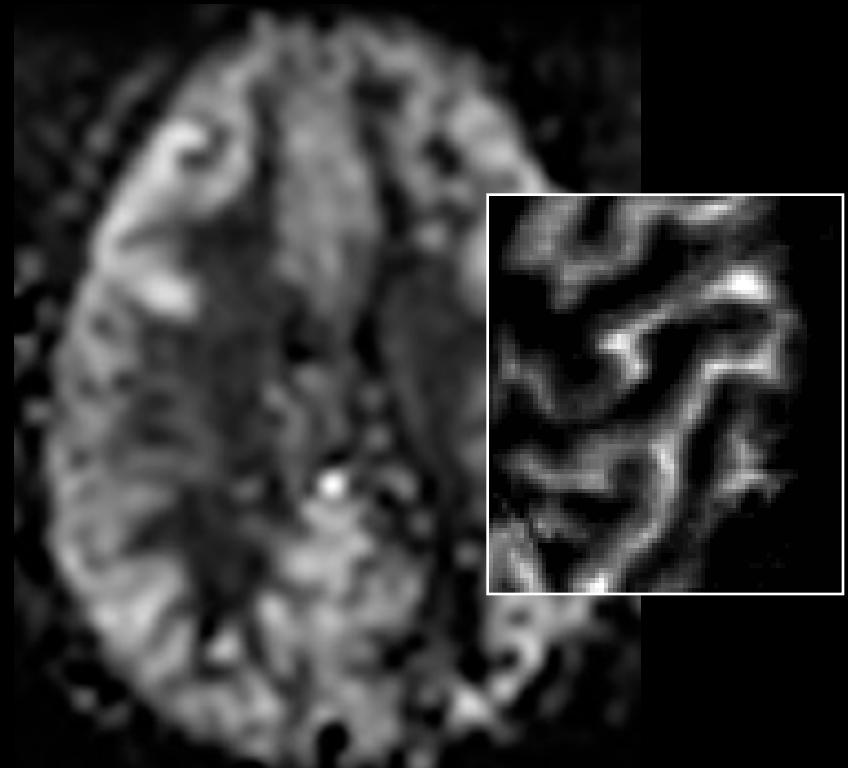
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# Comparison with Positron Emission Tomography



PET:  $\text{H}_2^{15}\text{O}$



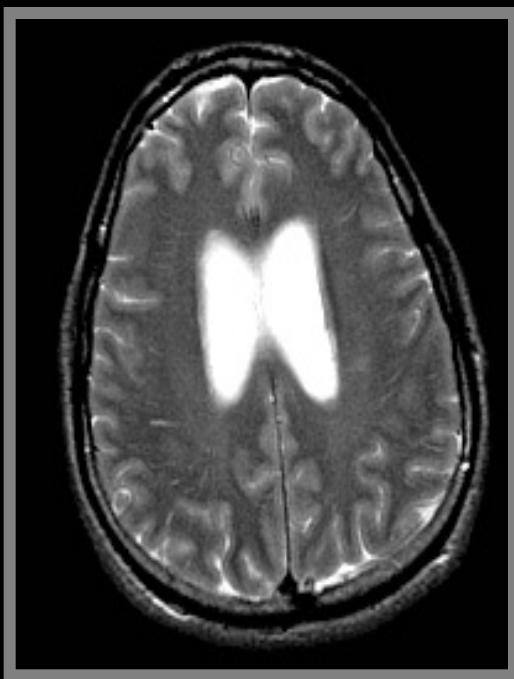
MRI: ASL

# Pushing the Envelope...

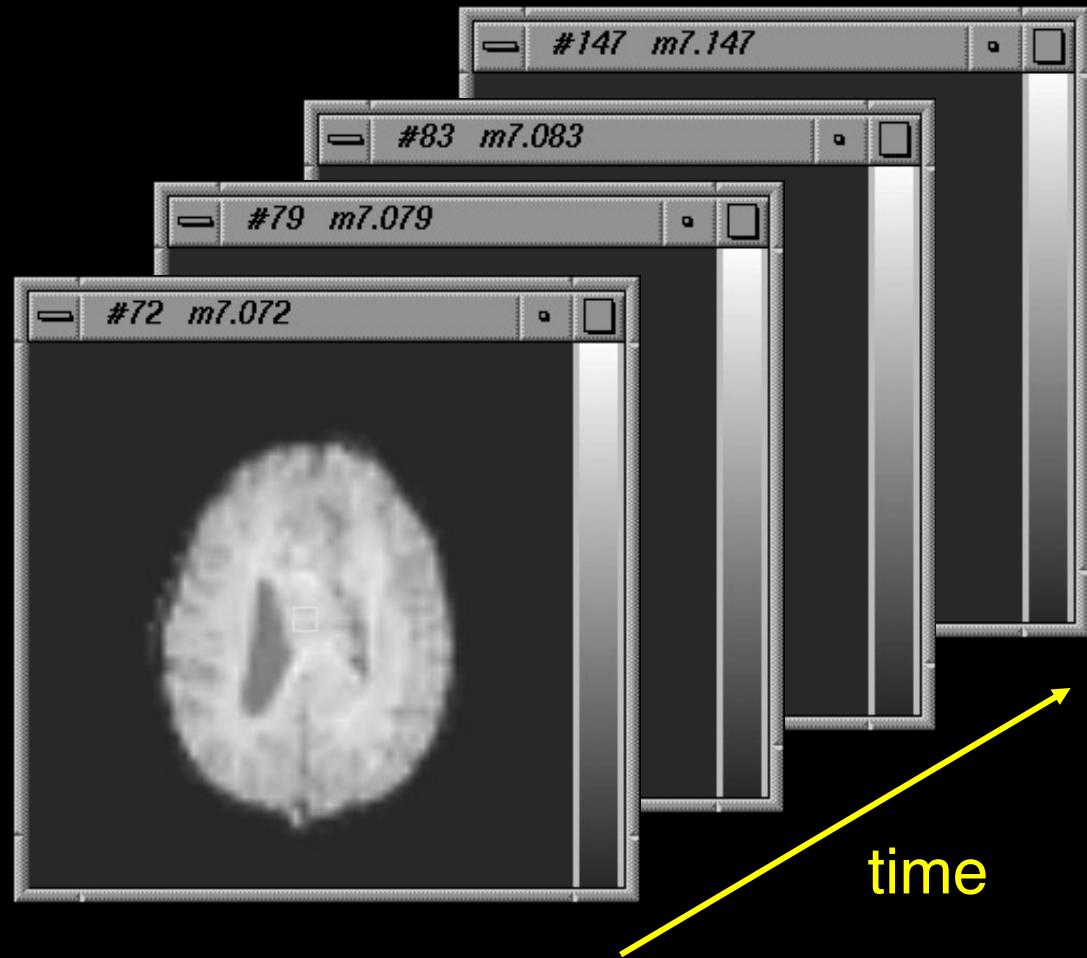
1. Temporal Resolution
2. Spatial Resolution
3. Sensitivity and Noise
4. Information Content
5. Implementation

# Pushing the Envelope...

1. Temporal Resolution
2. Spatial Resolution
3. Sensitivity and Noise
4. Information Content
5. Implementation

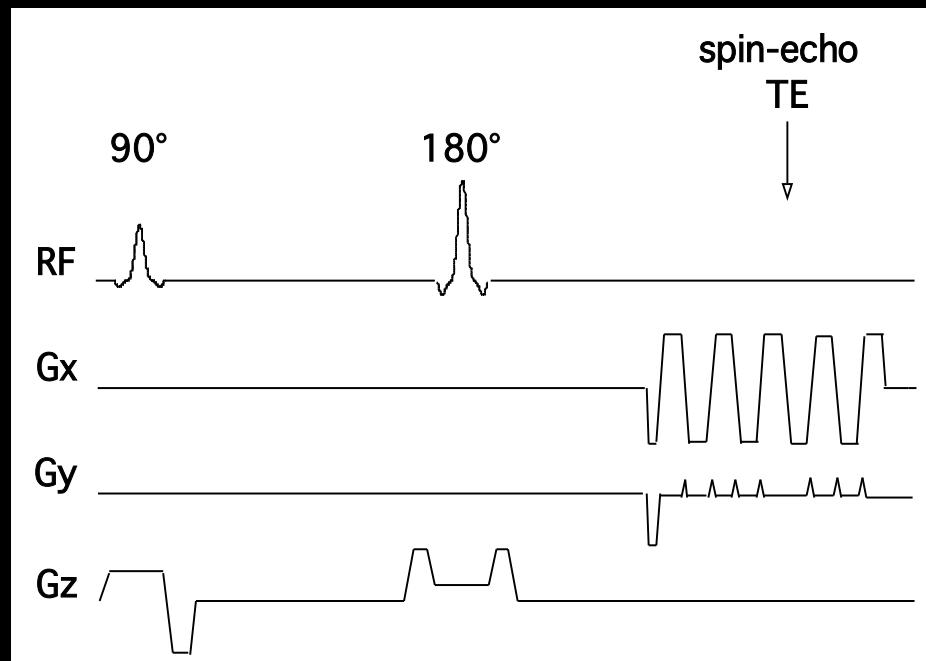
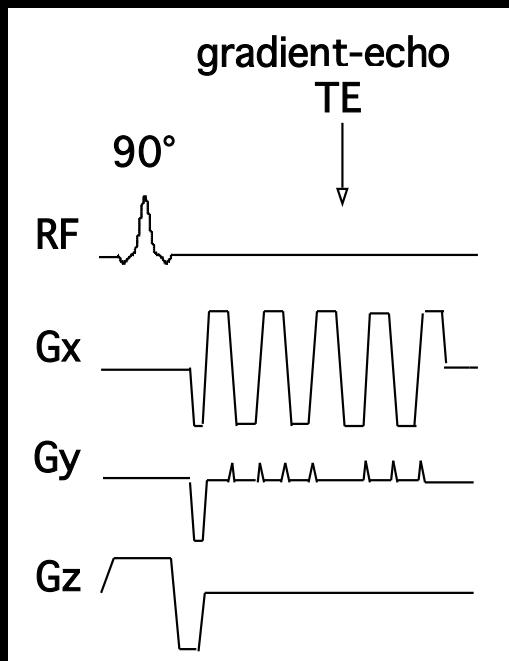


Anatomic

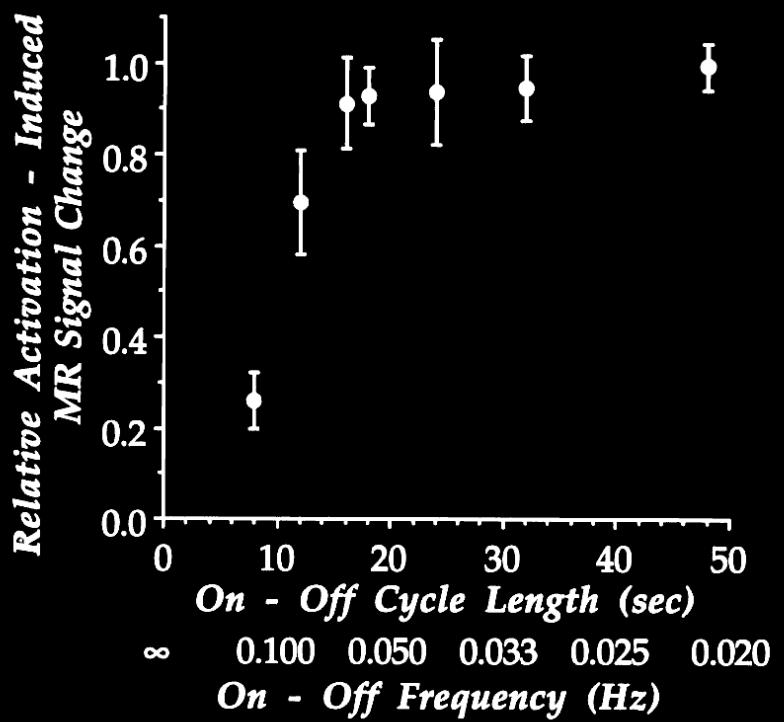
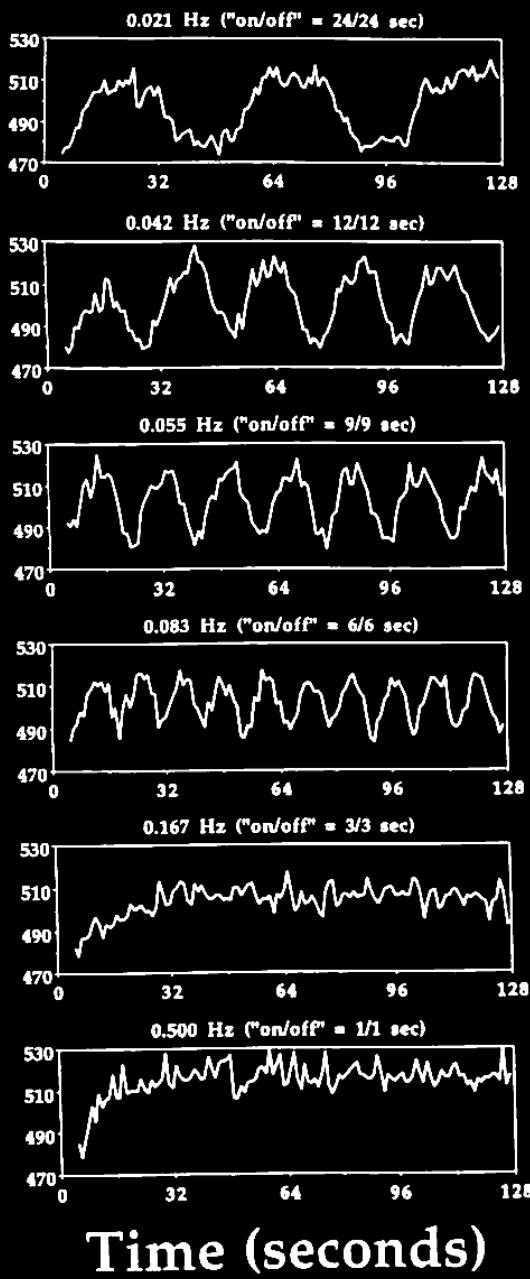


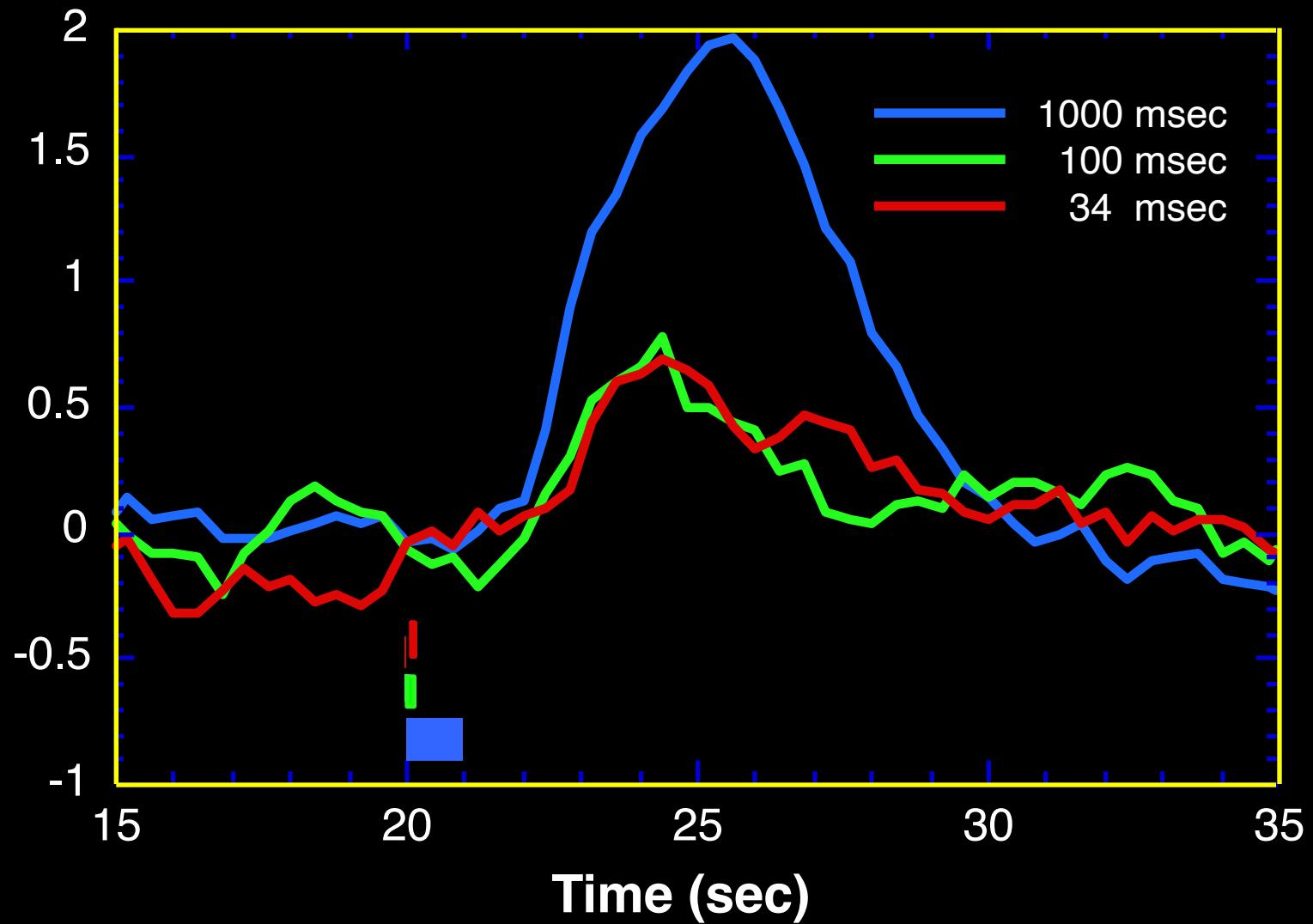
Functional

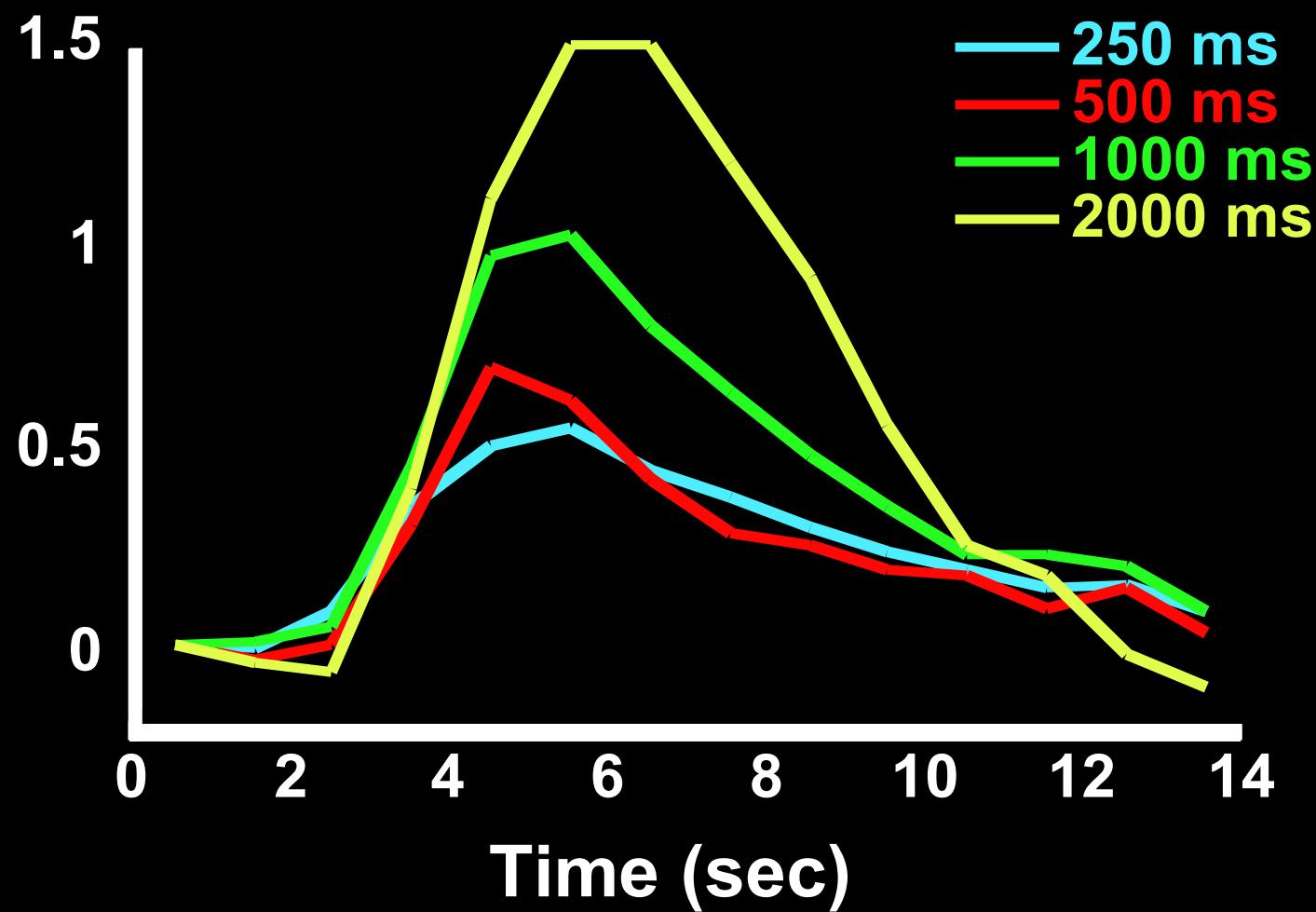
# Echo-Planar Imaging



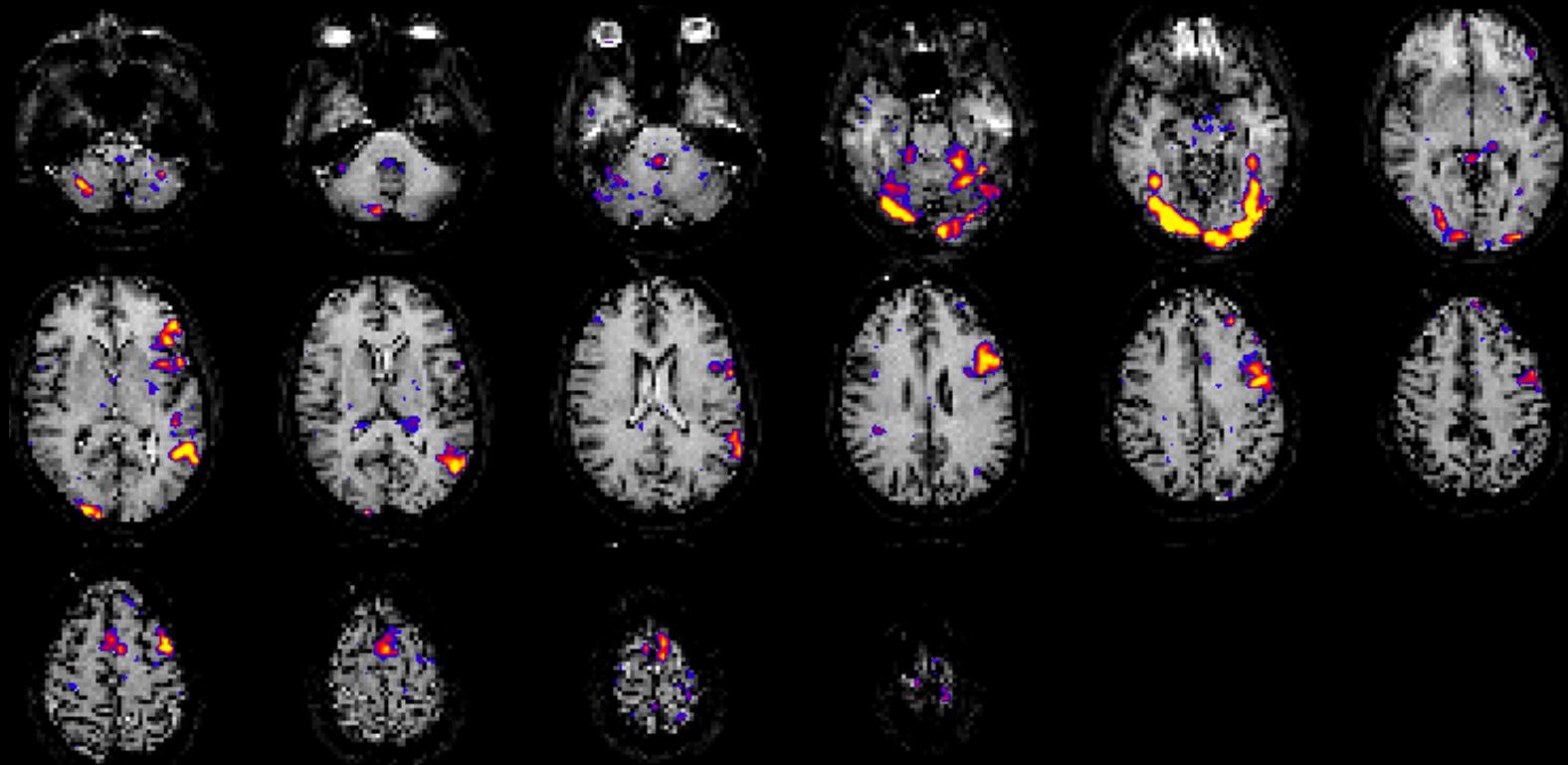
# MRI Signal



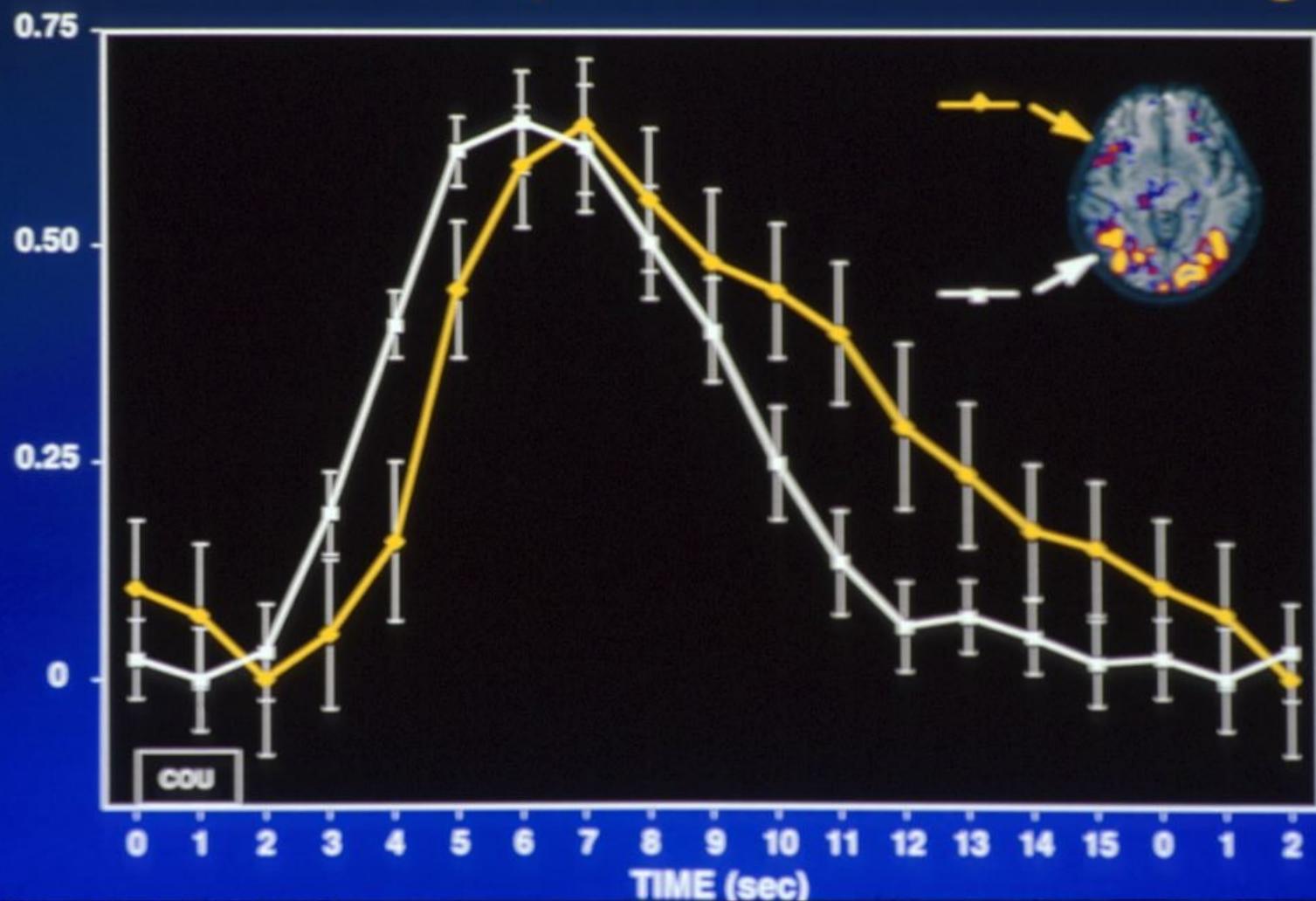




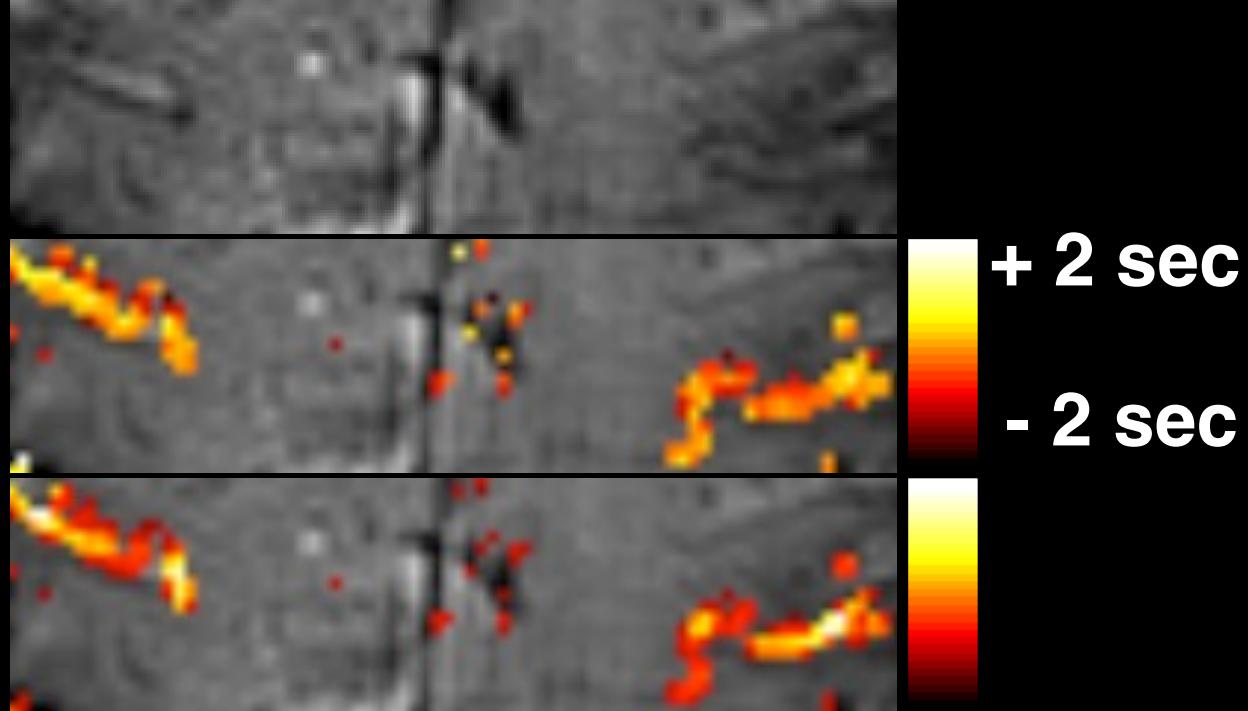
# Word stem completion



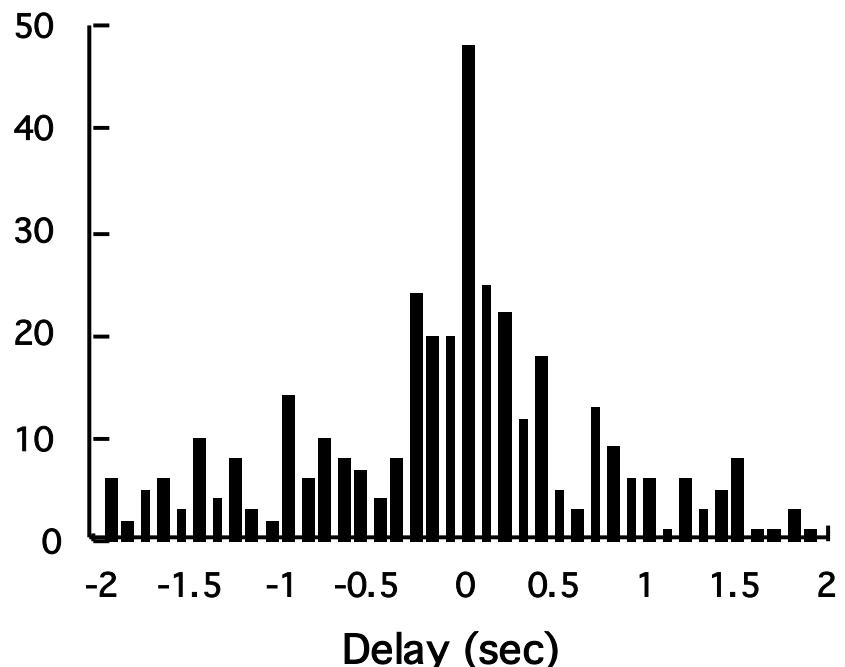
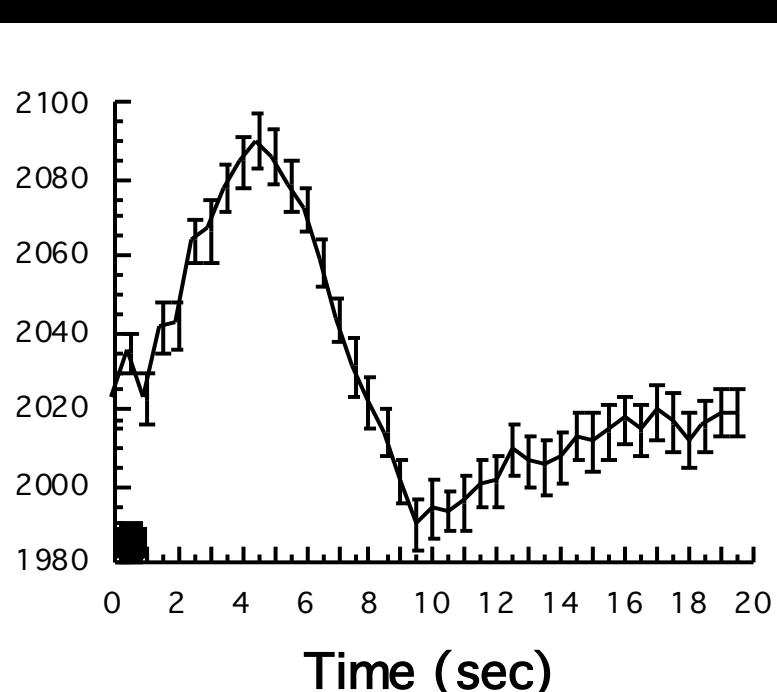
## Time Course Comparison Across Brain Regions



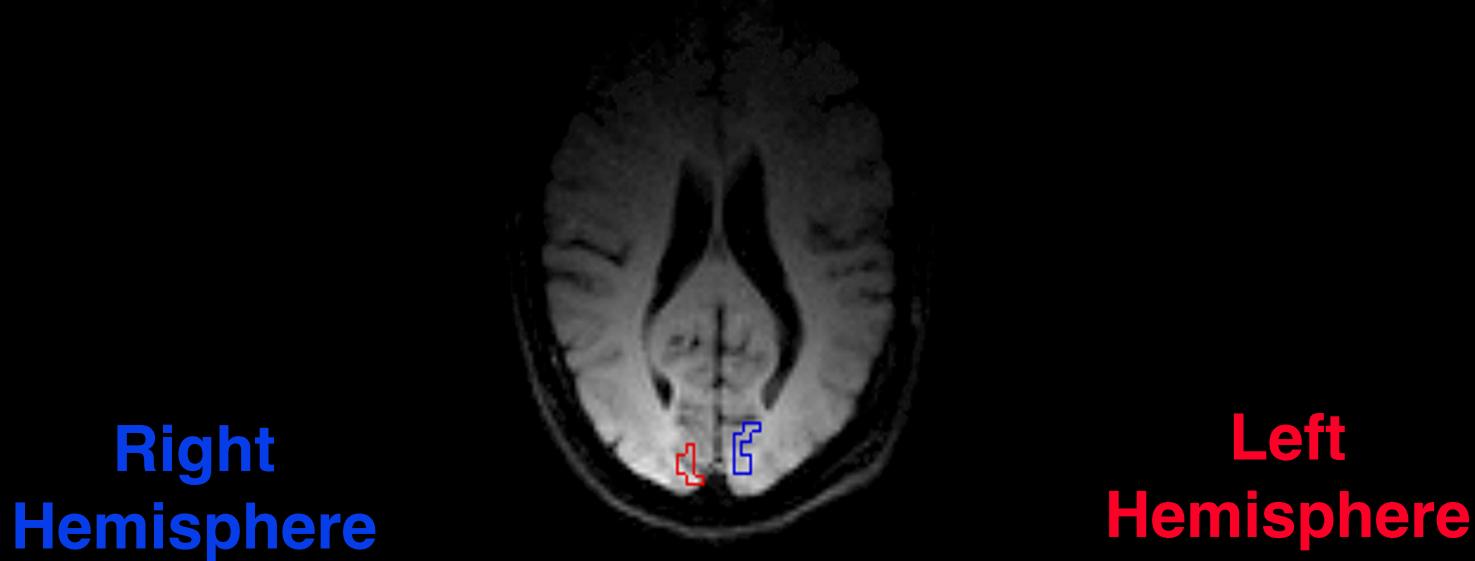
# Latency

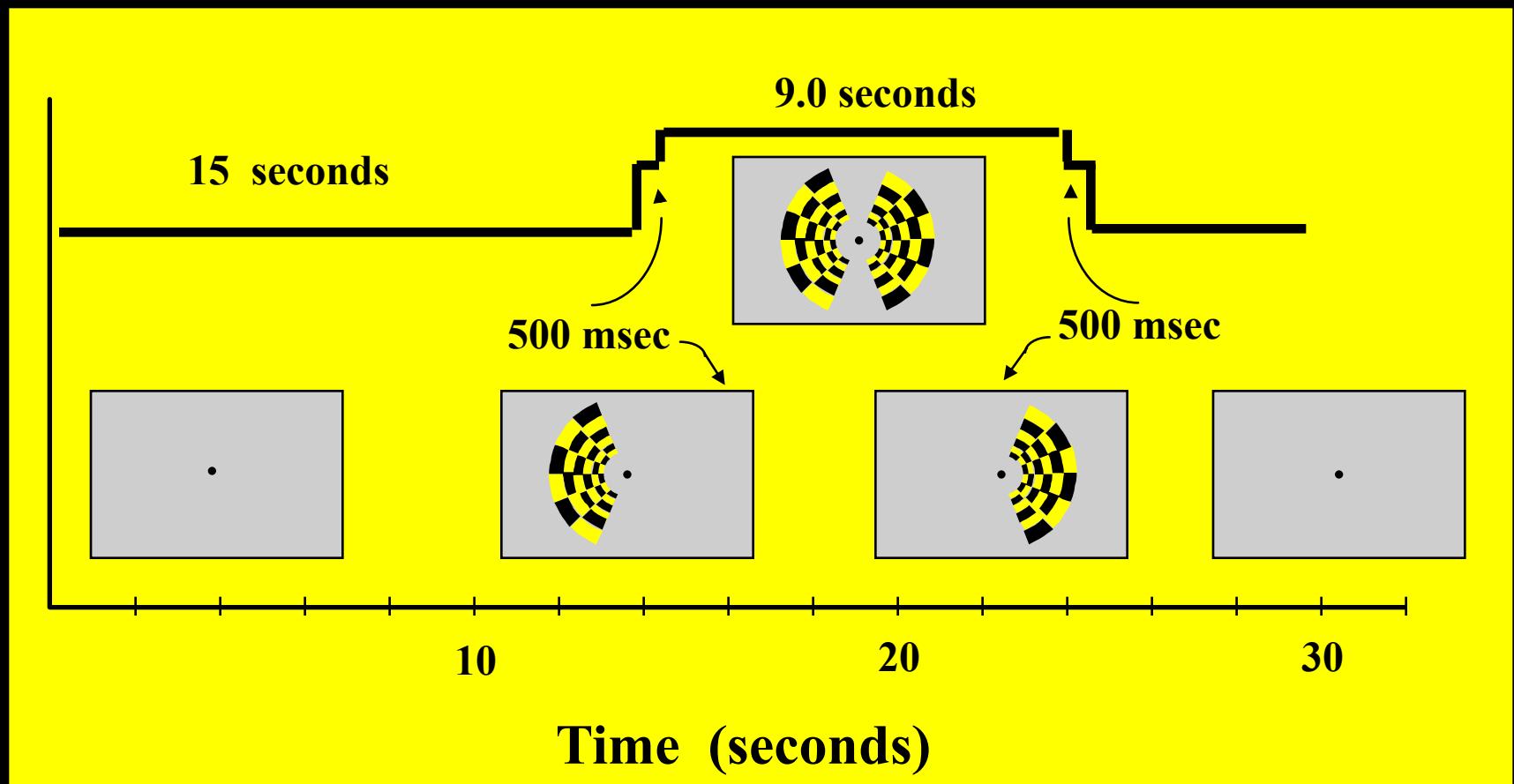


# Magnitude



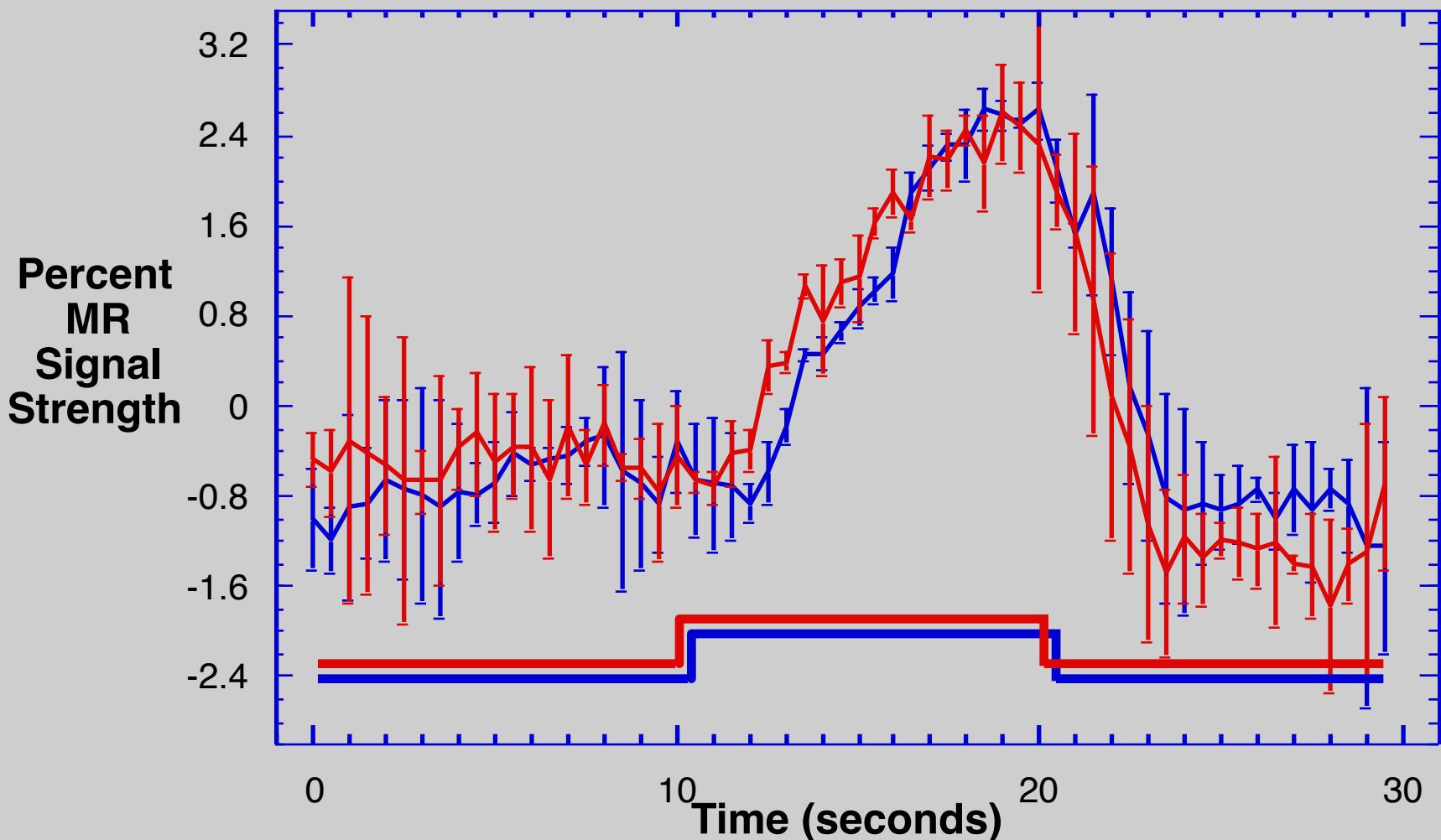
# Regions of Interest Used for Hemi-Field Experiment

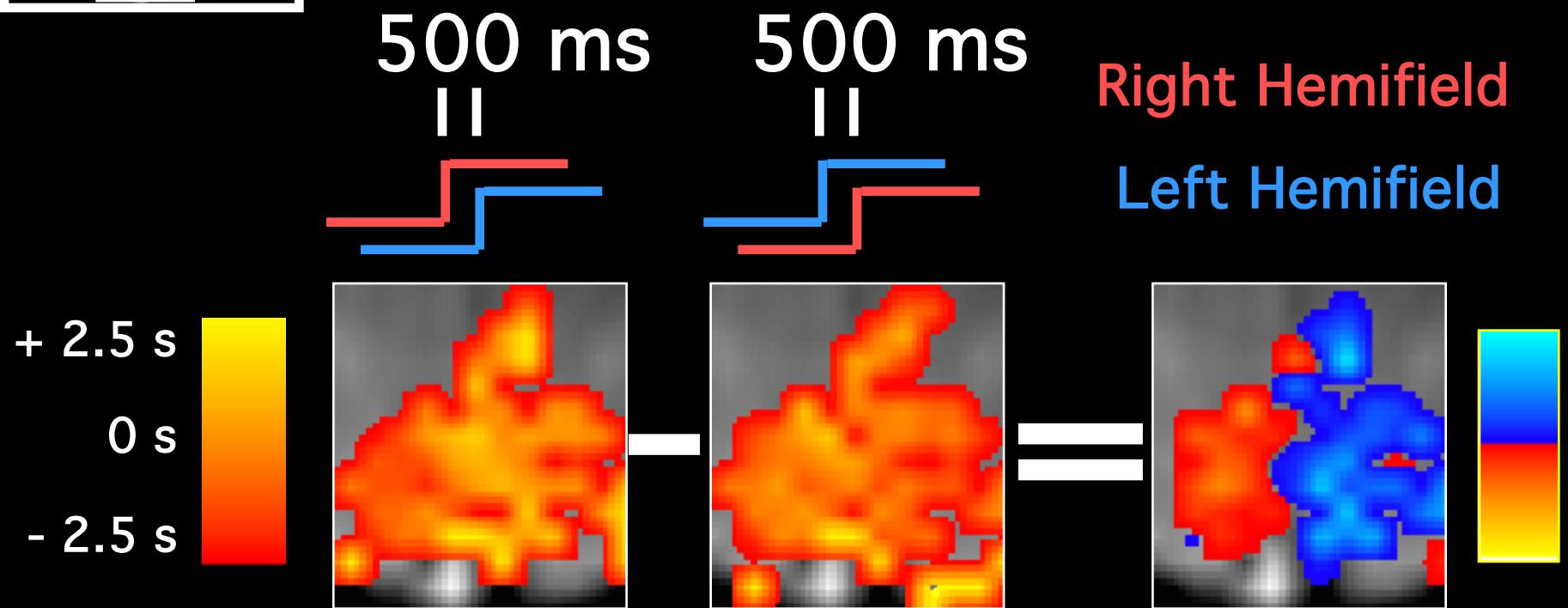
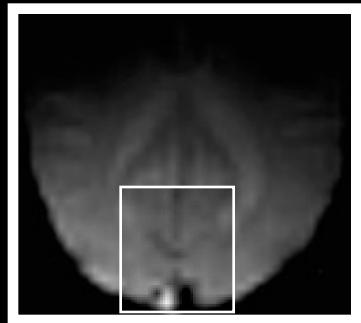




# Hemi-field with 500 msec asynchrony

Average of 6 runs    Standard Deviations Shown

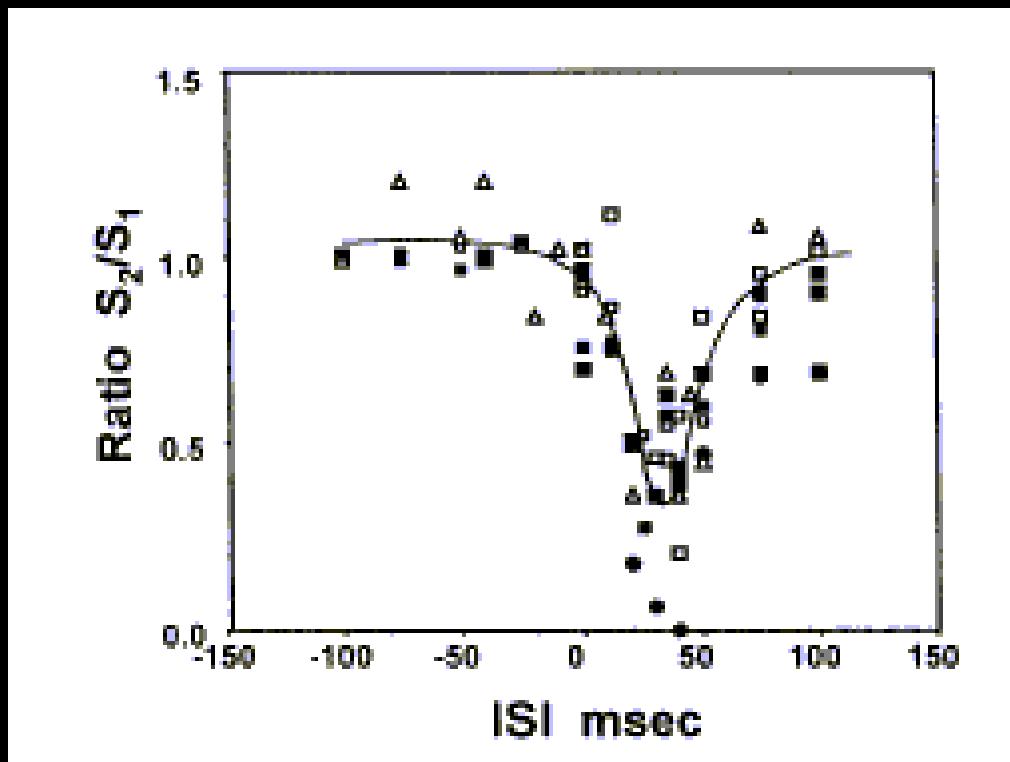




# An approach to probe some neural systems interaction by functional MRI at neural time scale down to milliseconds

Selji Ogawa<sup>1</sup>, Tso-Ming Lee<sup>1</sup>, Ray Stepnoski<sup>1</sup>, Wei Chen<sup>2</sup>, Xiao-Hong Zhu<sup>2</sup>, and Kamil Ugurbil<sup>2</sup>

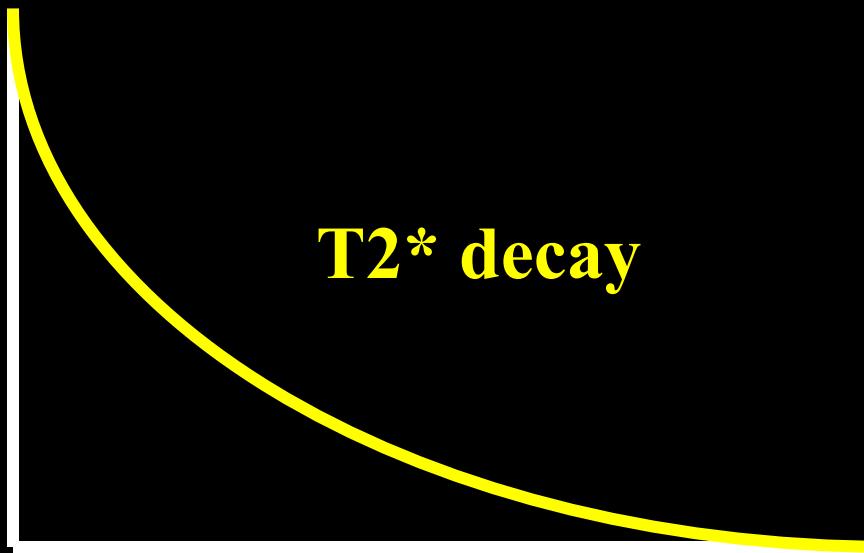
<sup>1</sup>Bell Laboratories, Lucent Technologies, Murray Hill, NJ 07974; and <sup>2</sup>Center for Magnetic Resonance Research, University of Minnesota Medical School, Minneapolis, MN 55455



# Pushing the Envelope...

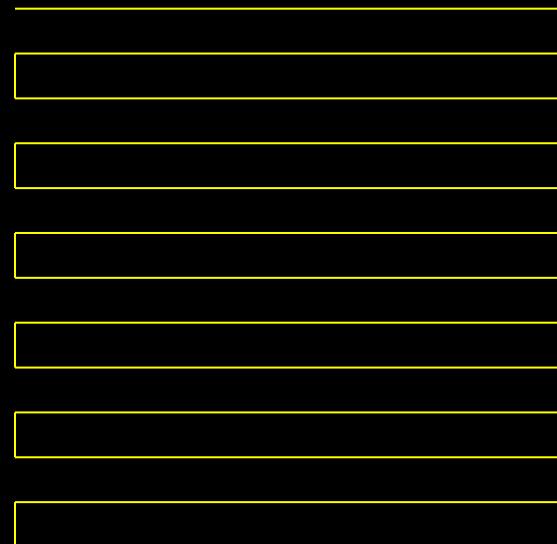
1. Temporal Resolution
2. Spatial Resolution
3. Sensitivity and Noise
4. Information Content
5. Implementation

# Single Shot Imaging



EPI Readout Window

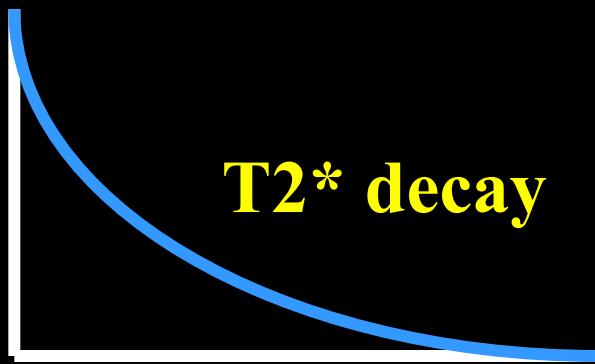
$\approx 20$  to 40 ms



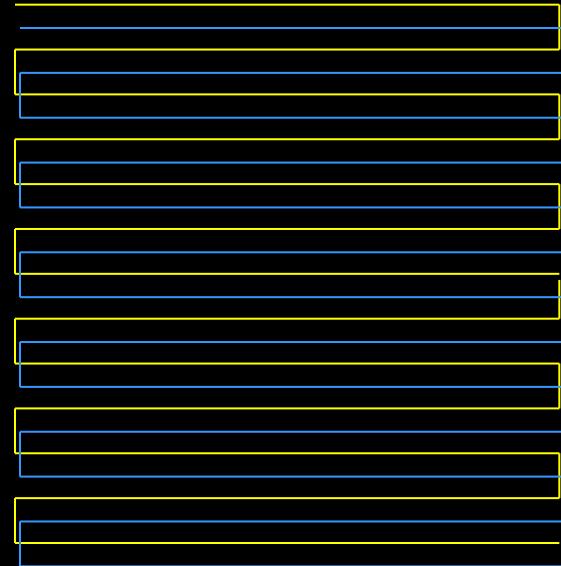
# Multishot Imaging



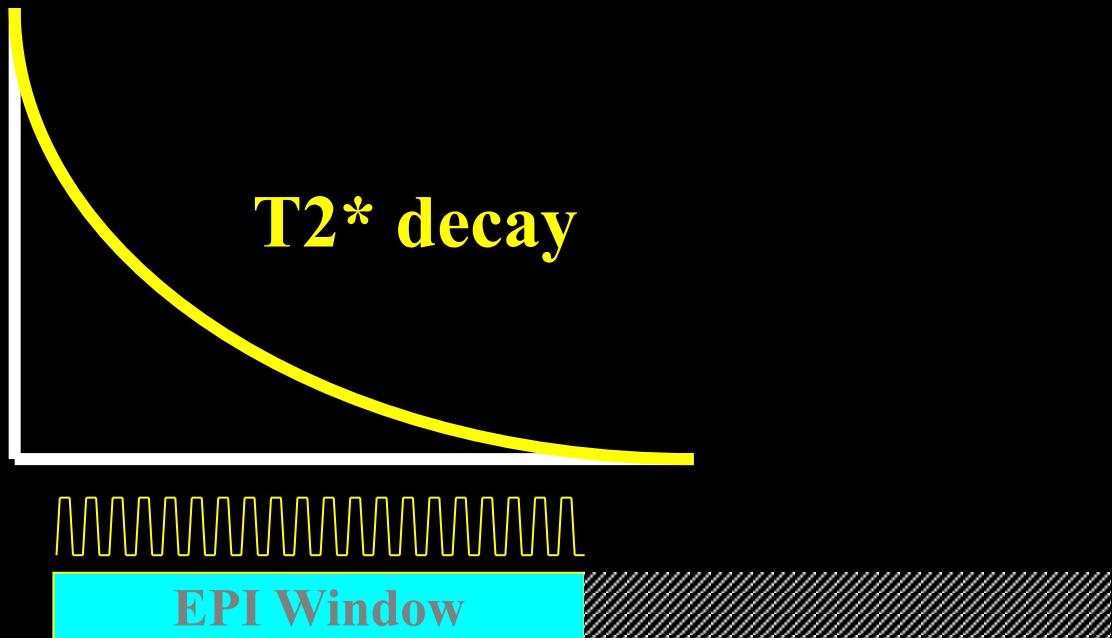
EPI Window 1



EPI Window 2



# Partial k-space imaging



# Multi Shot EPI

Excitations

1

Matrix Size

64 x 64

2

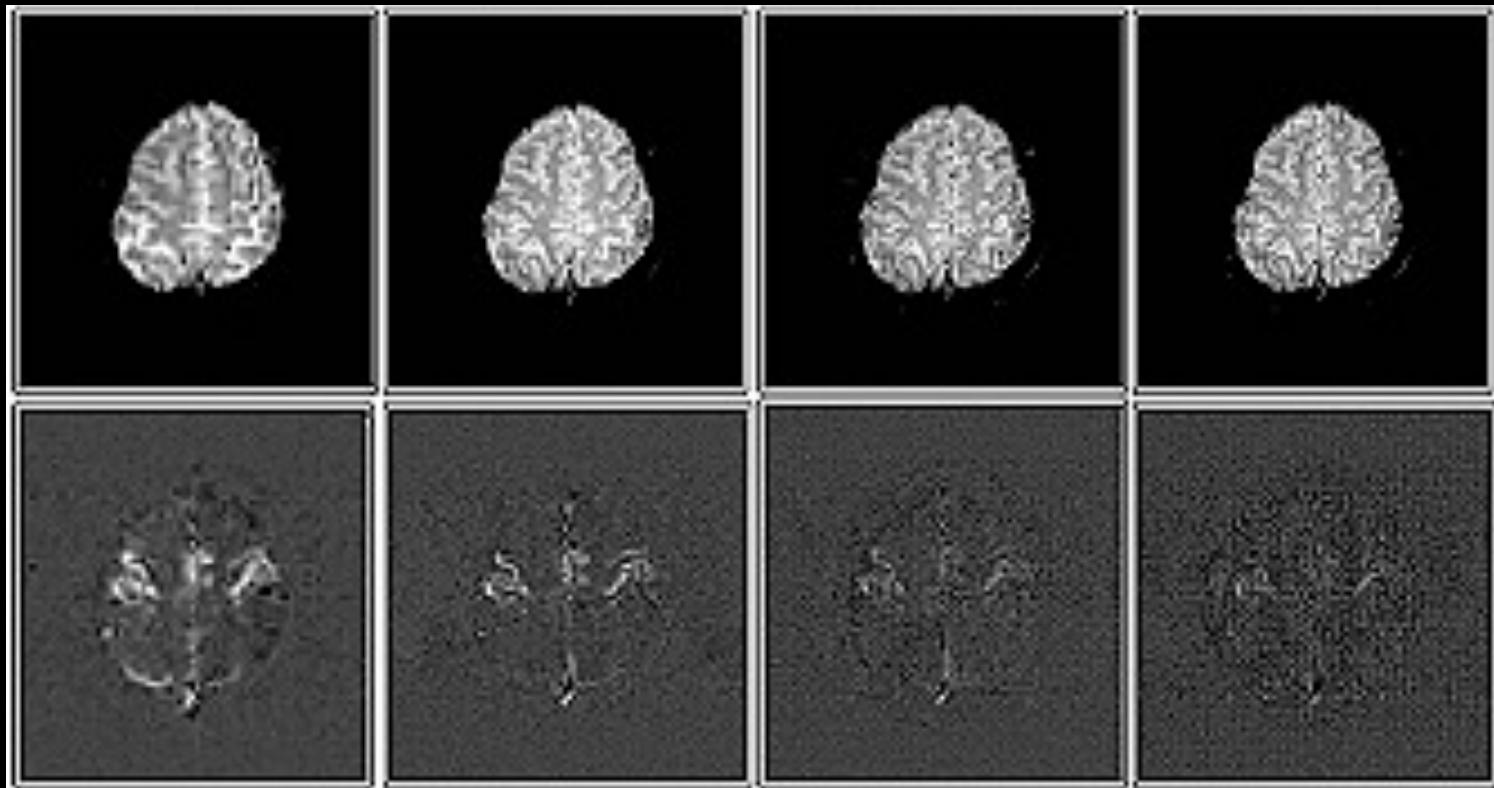
128 x 128

4

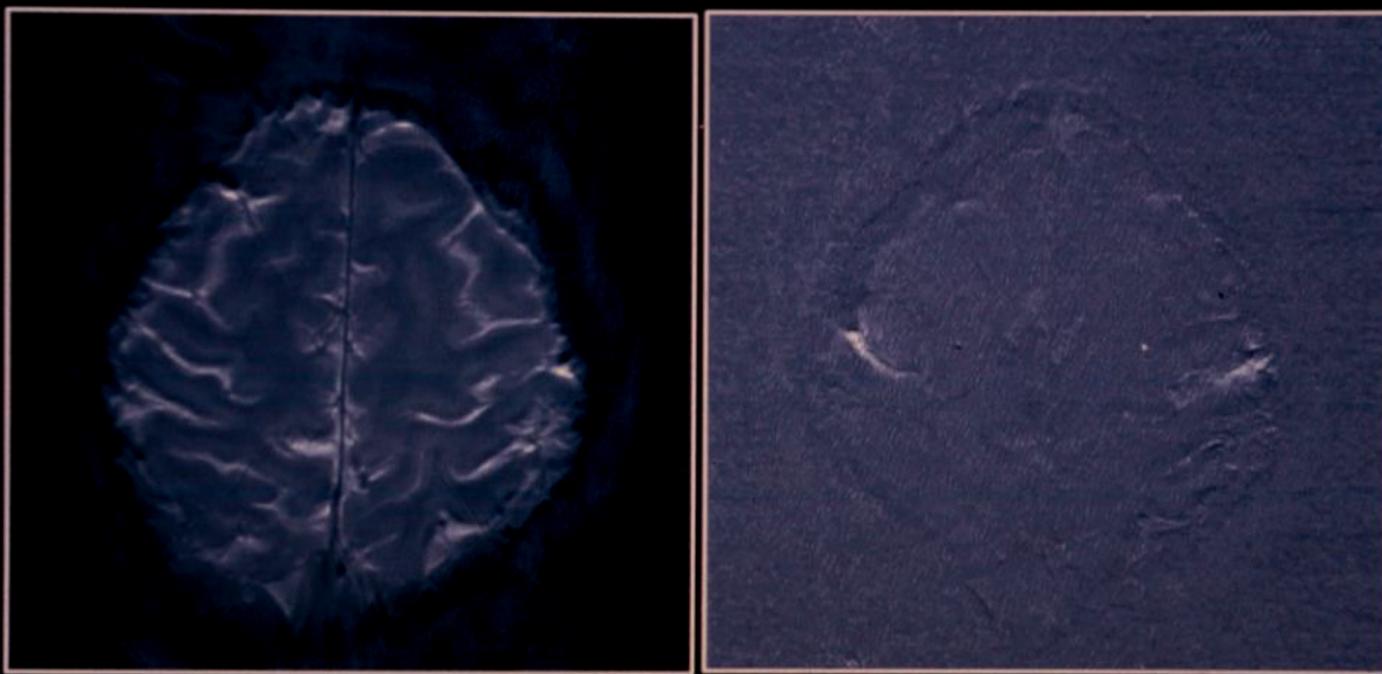
256 x 128

8

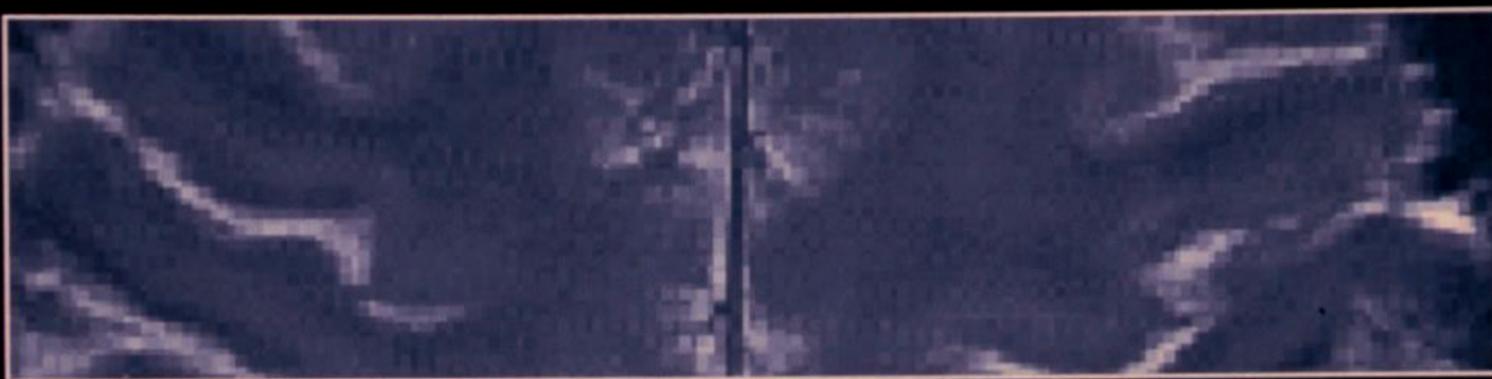
256



**Single - Shot EPI at 3T:  
Half NEX, 256 x 256, 16 cm FOV**

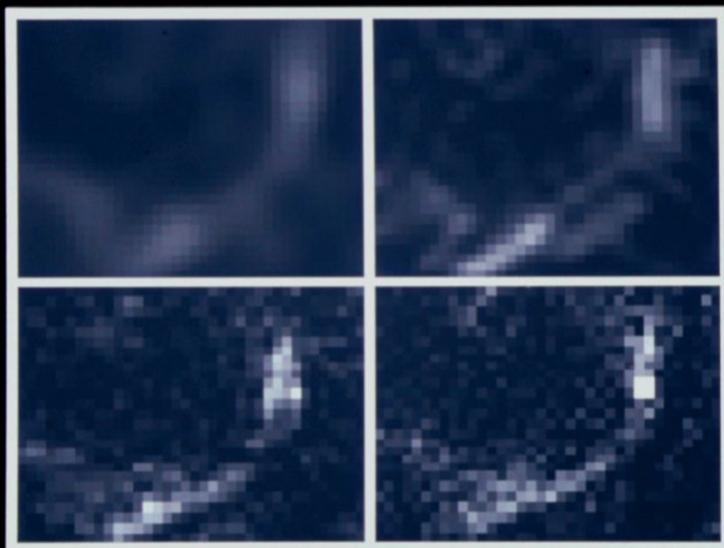


**Single - Shot EPI at 3T:  
Half NEX 256 x 256, 16 cm FOV**



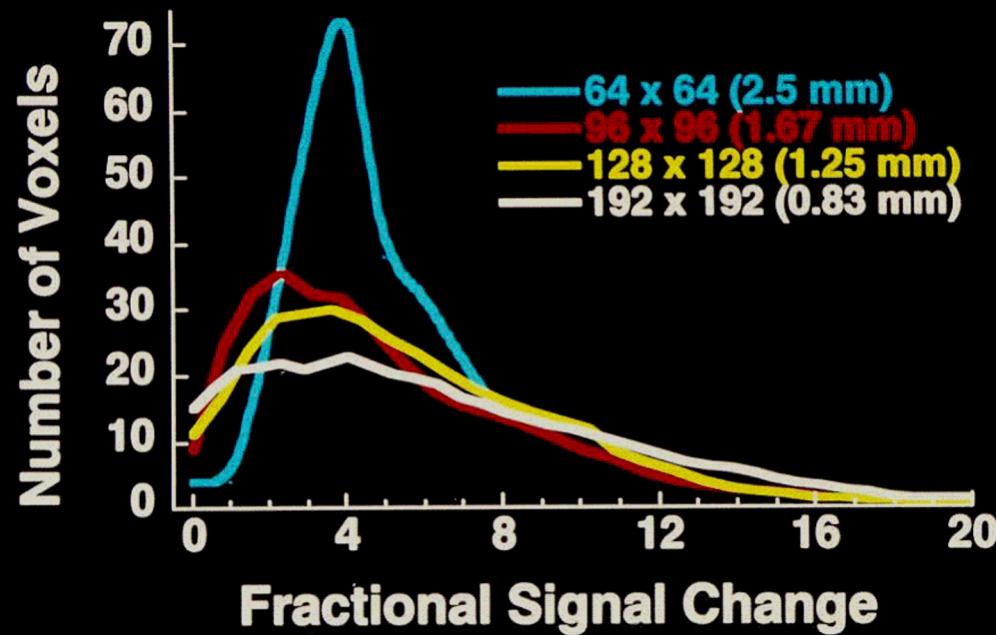
## Fractional Signal Change

$2.5 \text{ mm}^2$



$1.25 \text{ mm}^2$

$0.62 \text{ mm}^2$

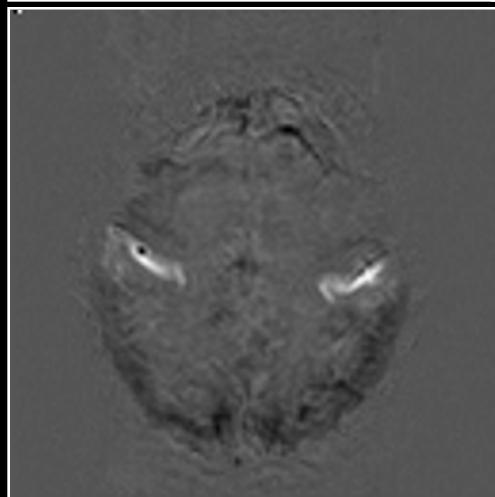
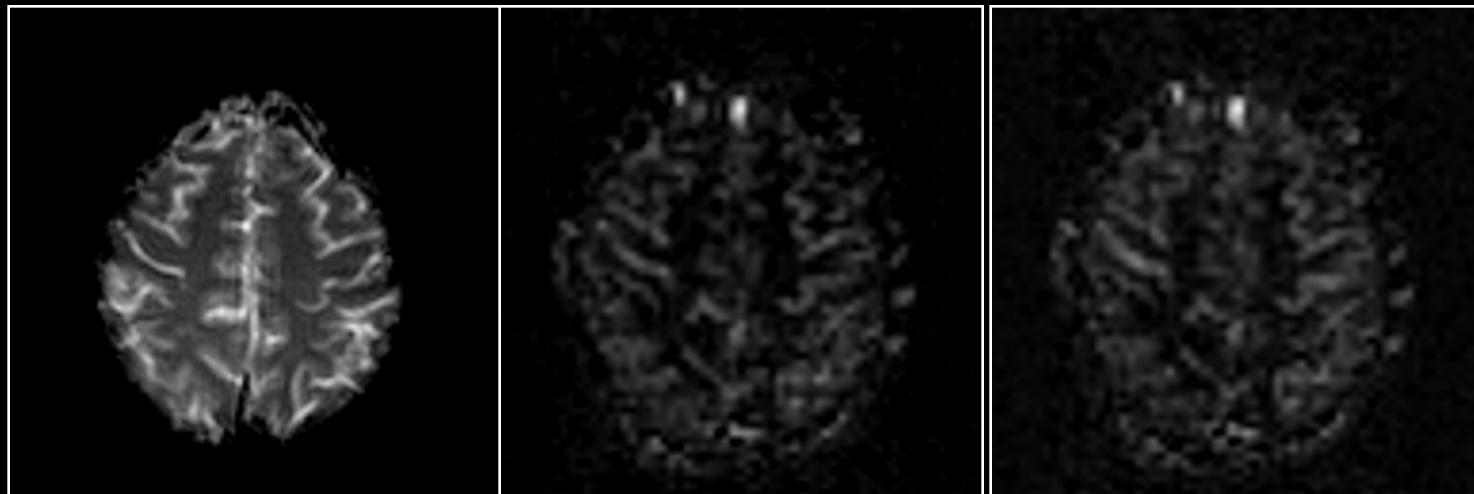


# Perfusion

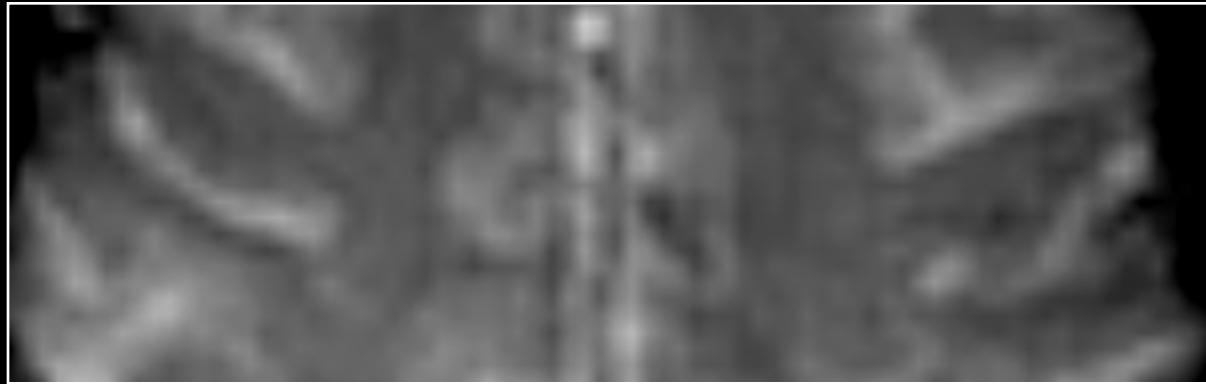
**BOLD**

*Rest*

*Activation*



# **Anatomy**



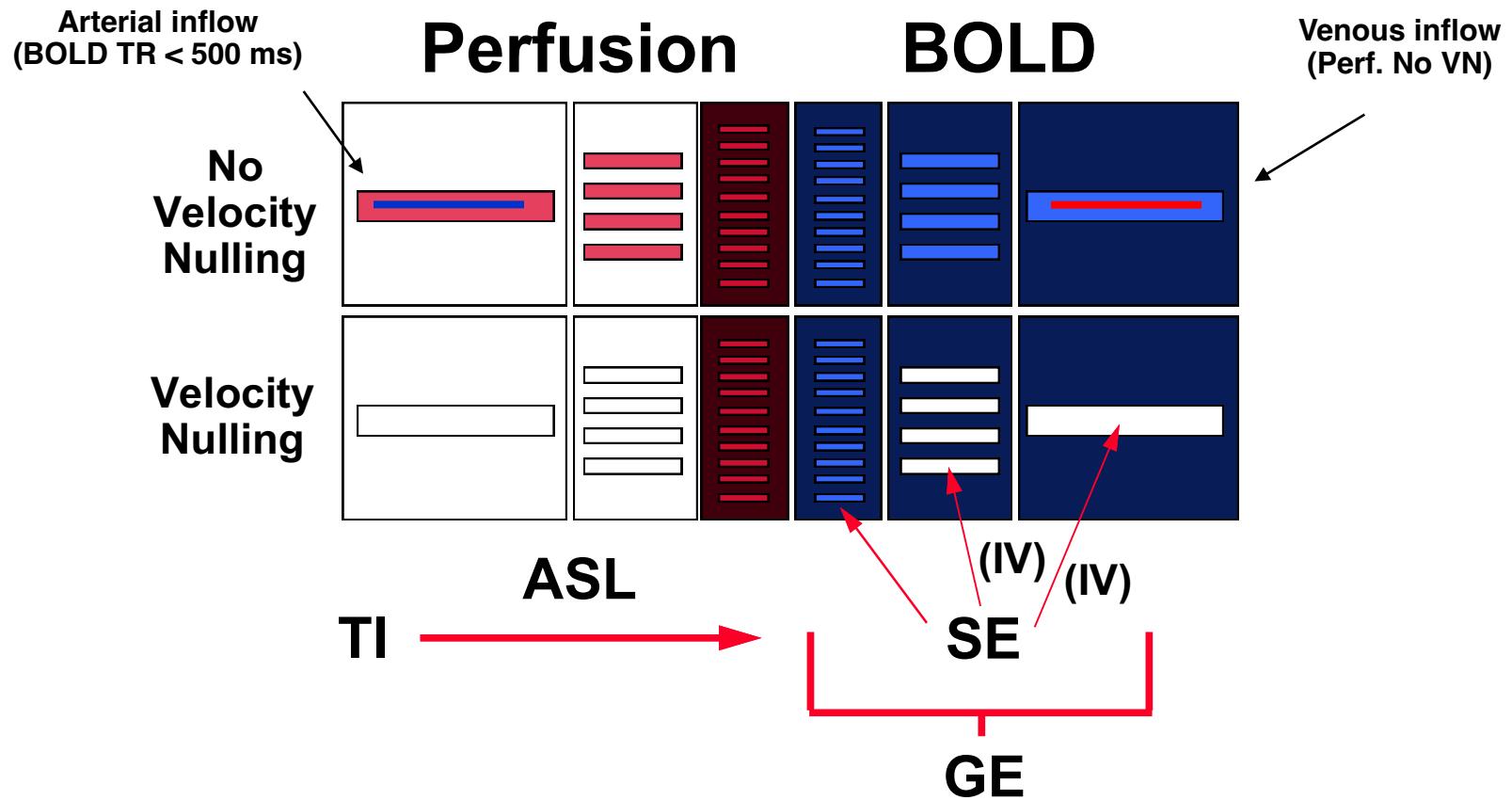
# **BOLD**



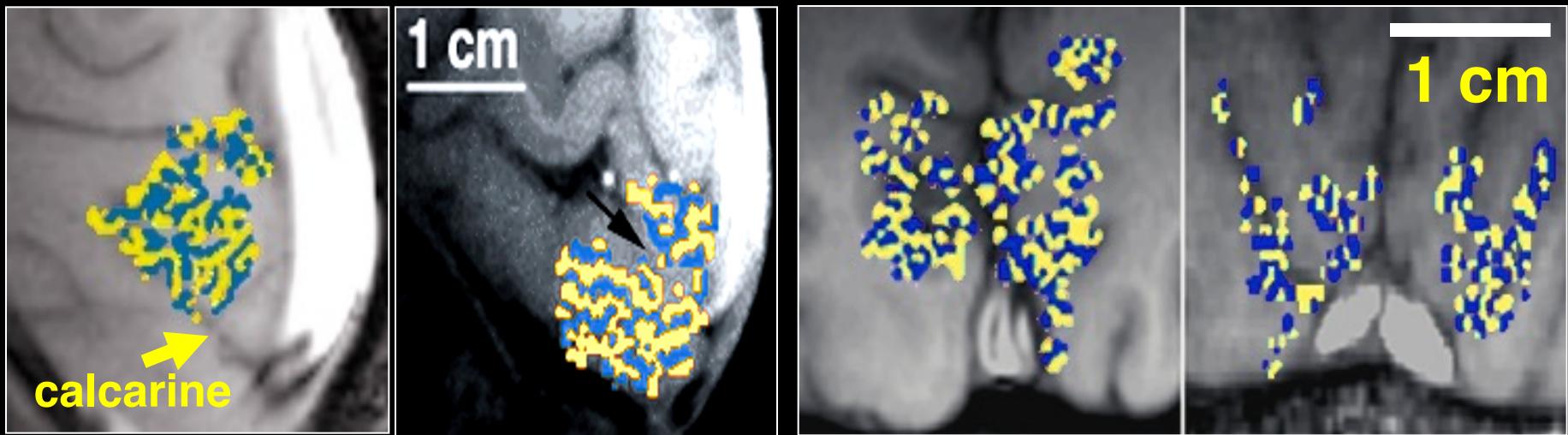
# **Perfusion**



# Hemodynamic Specificity



# ODC Maps using fMRI



- Identical in size, orientation, and appearance to those obtained by optical imaging<sup>1</sup> and histology<sup>3,4</sup>.

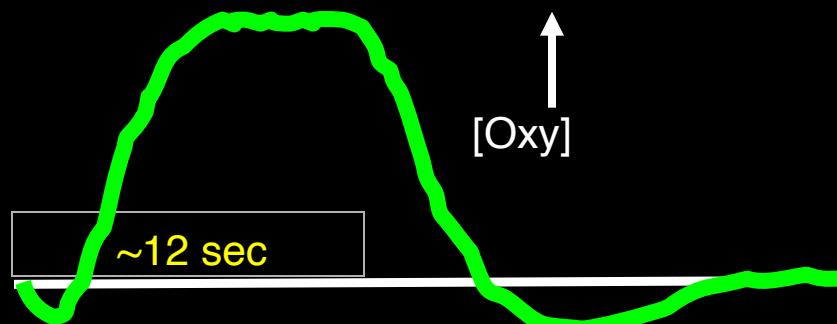
<sup>1</sup>Malonek D, Grinvald A. *Science* 272, 551-4 (1996).

<sup>3</sup>Horton JC, Hocking DR. *J Neurosci* 16, 7228-39 (1996).

<sup>4</sup>Horton JC, et al. *Arch Ophthalmol* 108, 1025-31 (1990).

# Why short is better than long

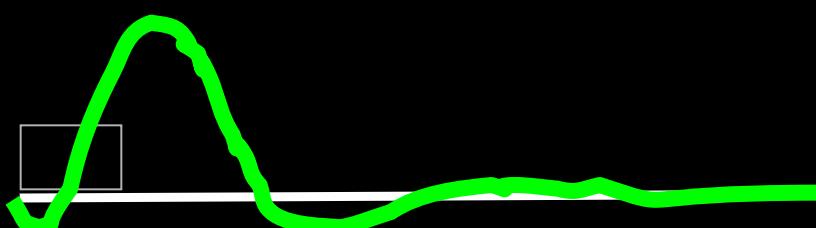
The vascular response to prolonged neural stimulation



It is argued that fMRI cannot achieve submillimeter functional resolution because a saturated hyperoxic vascular response to neural activity spreads over many millimeters<sup>1,2</sup>.

However, optical imaging has demonstrated that the hyperoxic response can yield well-localized maps when using short duration stimuli (<5 sec)<sup>1</sup>.

The vascular response to brief neural stimulation



<sup>1</sup>Malonek D, Grinvald A. Science 272, 551-4 (1996).

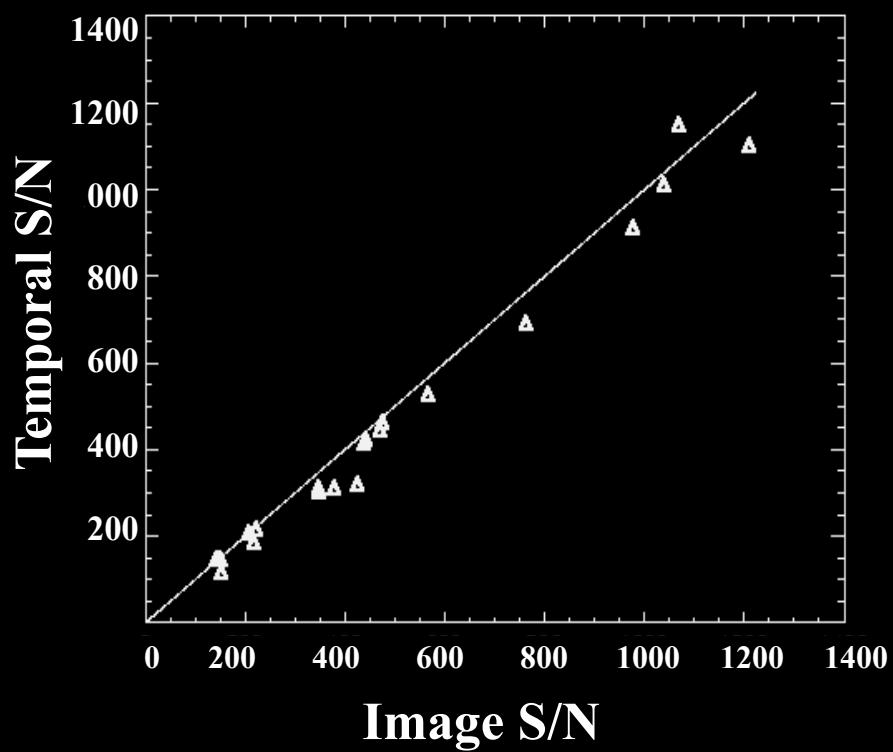
<sup>2</sup>Kim D-S, Duong T, Kim S-G. Nat Neurosci 3, 164-9 (2000).

# Pushing the Envelope...

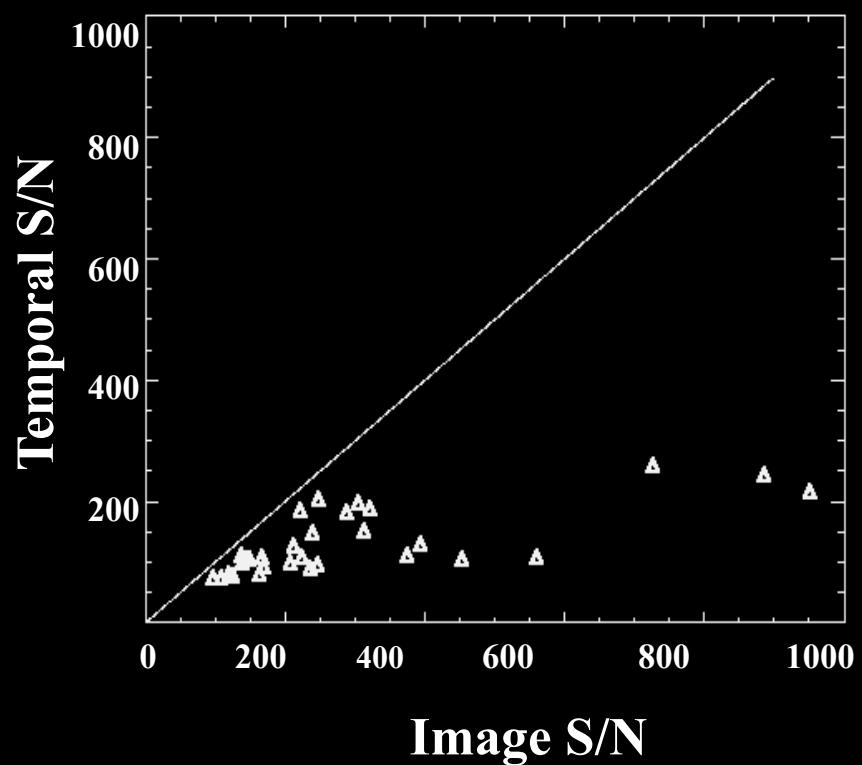
1. Temporal Resolution
2. Spatial Resolution
3. Sensitivity and Noise
4. Information Content
5. Implementation

# Temporal S/N vs. Image S/N

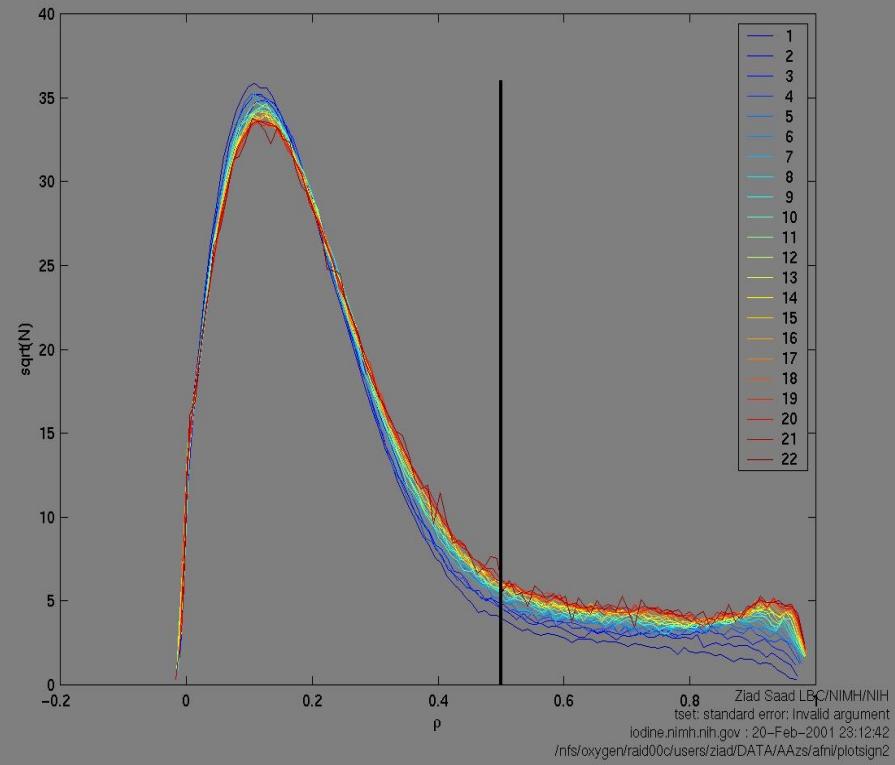
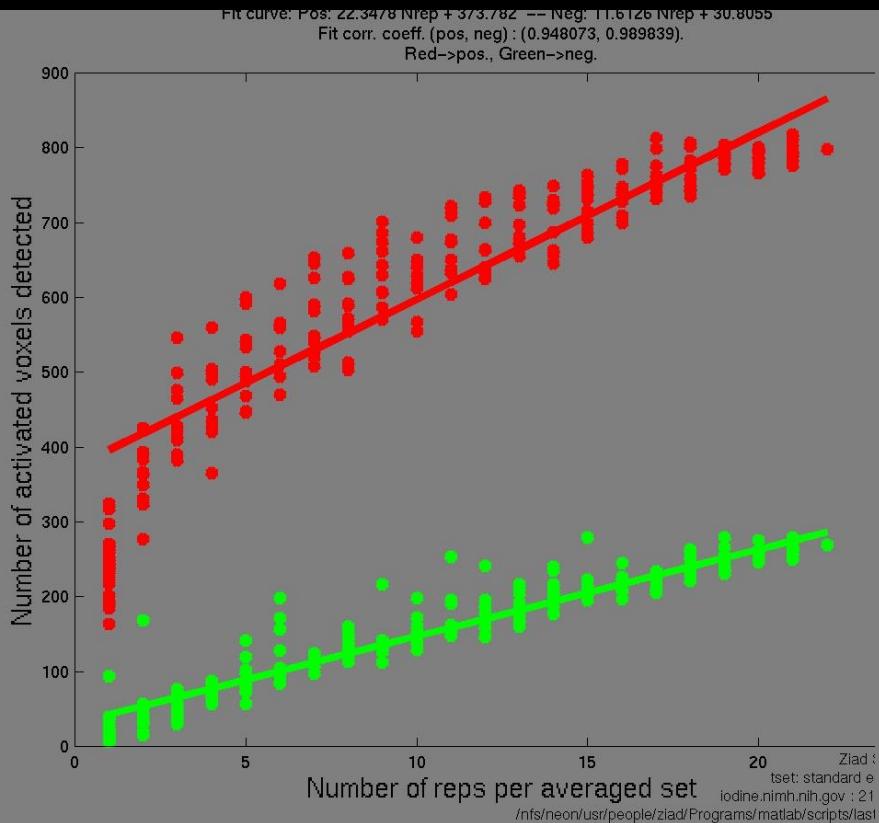
PHANTOMS



SUBJECTS



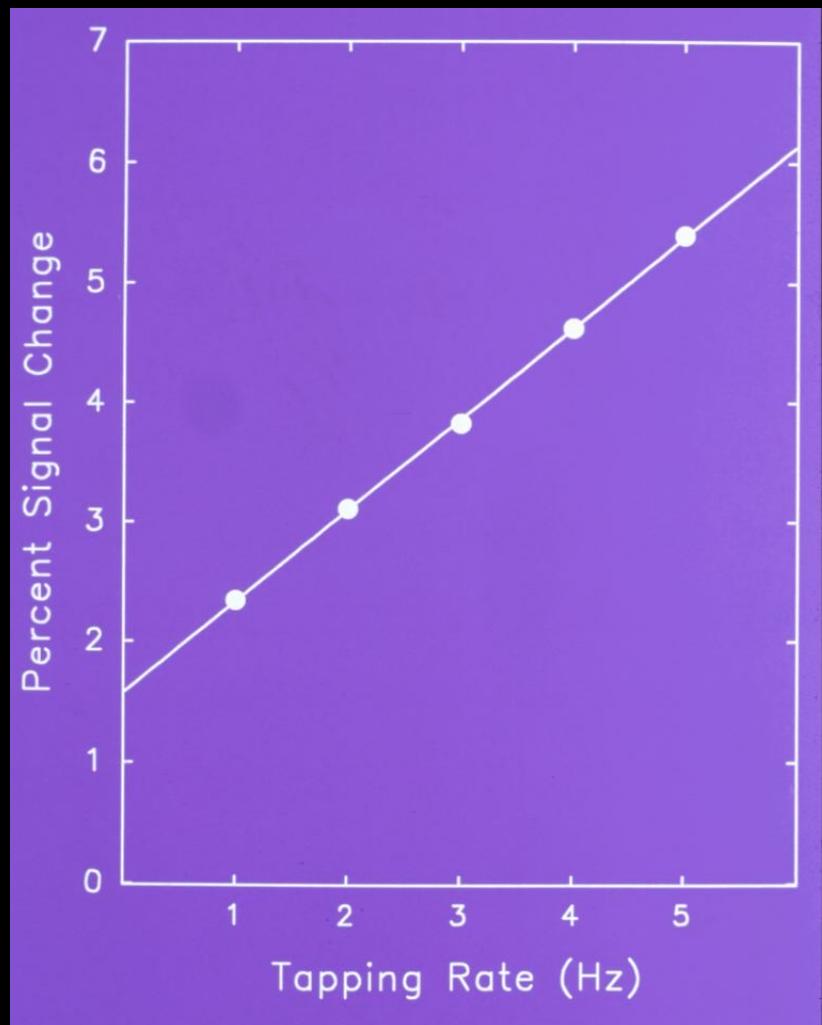
N. Petridou



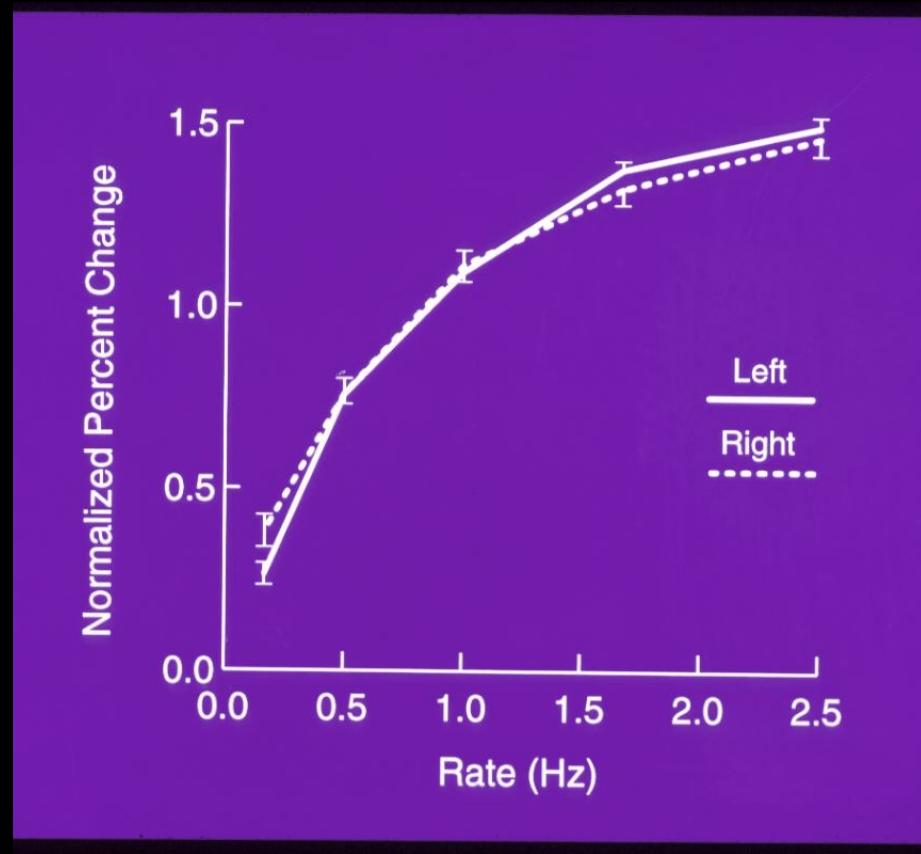
# Pushing the Envelope...

1. Temporal Resolution
2. Spatial Resolution
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- 4. Information Content**
5. Implementation

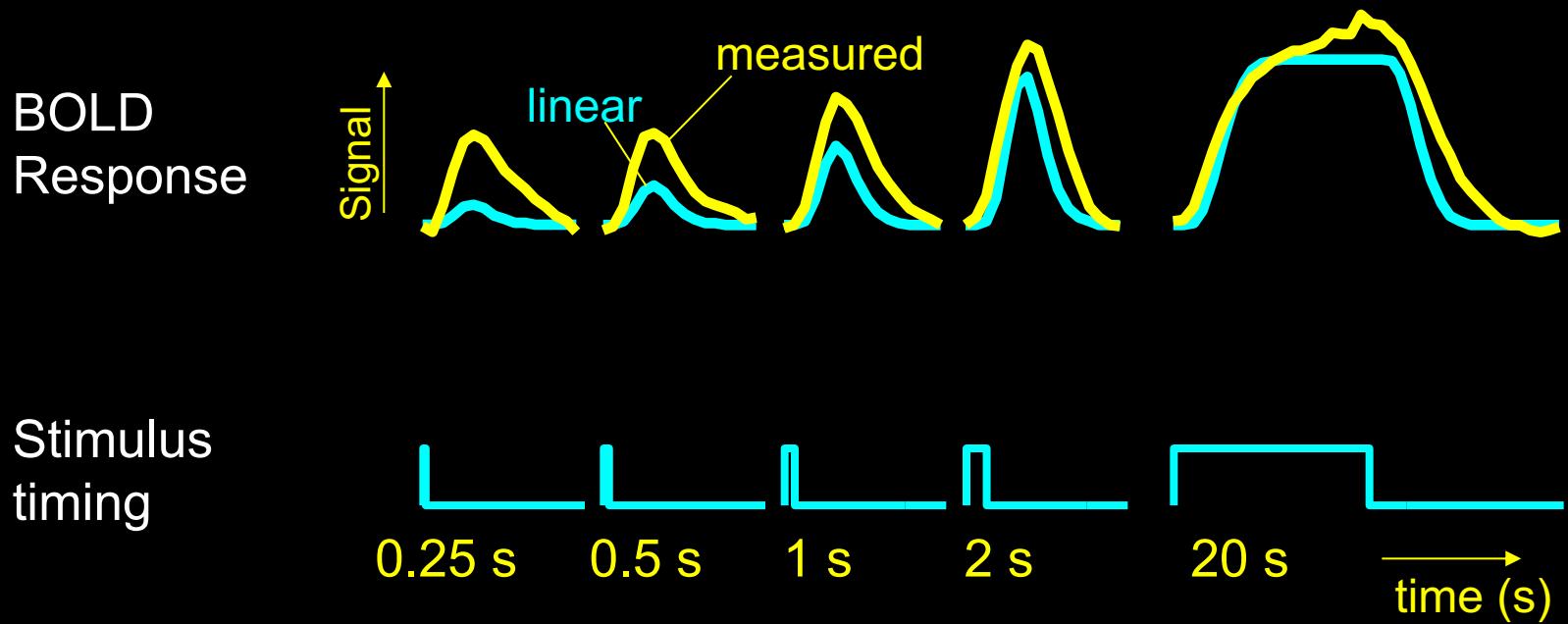
# Motor Cortex



# Auditory Cortex



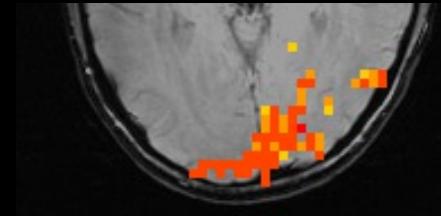
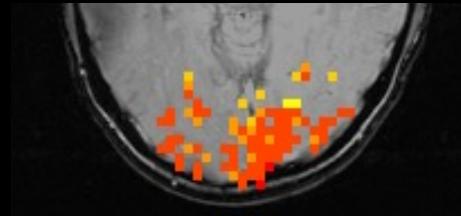
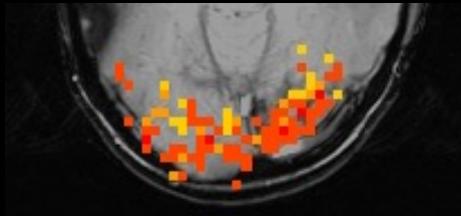
# Different stimulus “ON” periods



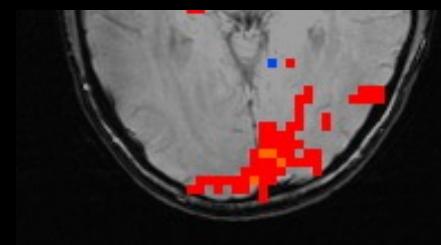
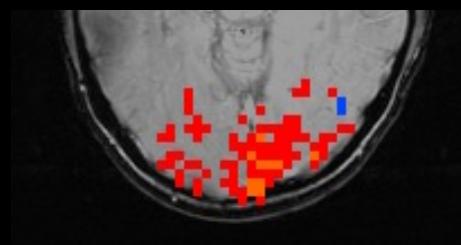
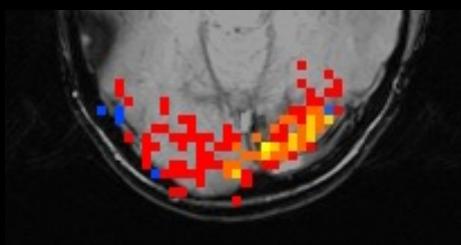
*Brief stimuli produce larger responses than expected*

# Results – visual task

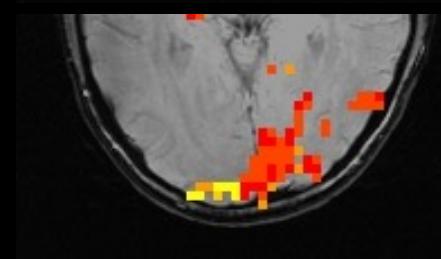
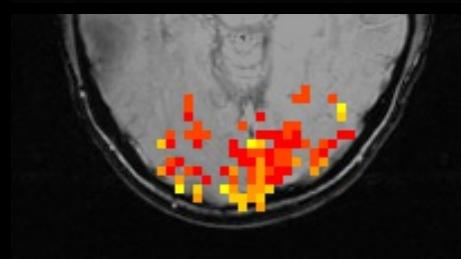
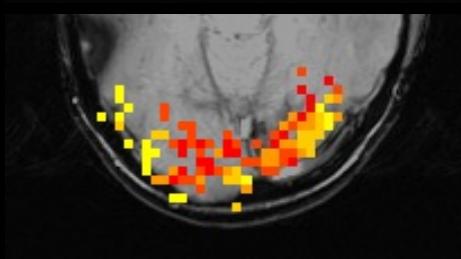
Nonlinearity



Magnitude

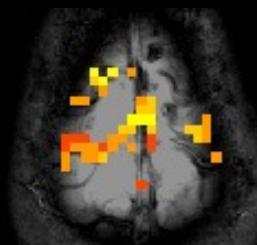
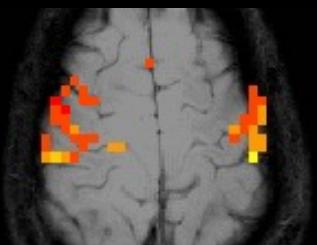
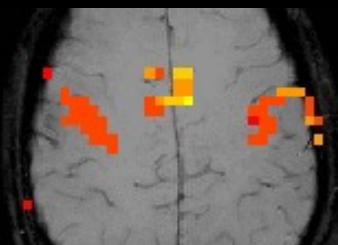


Latency

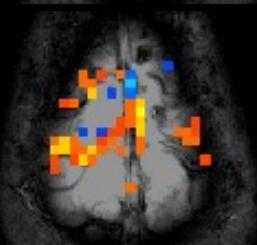
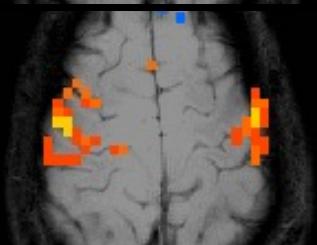
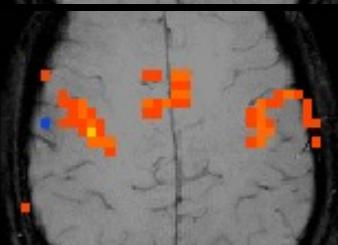


# Results – motor task

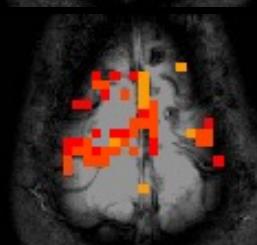
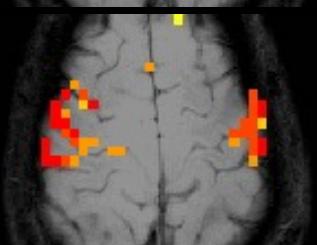
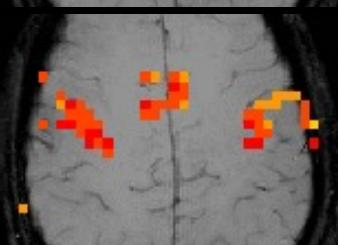
Nonlinearity



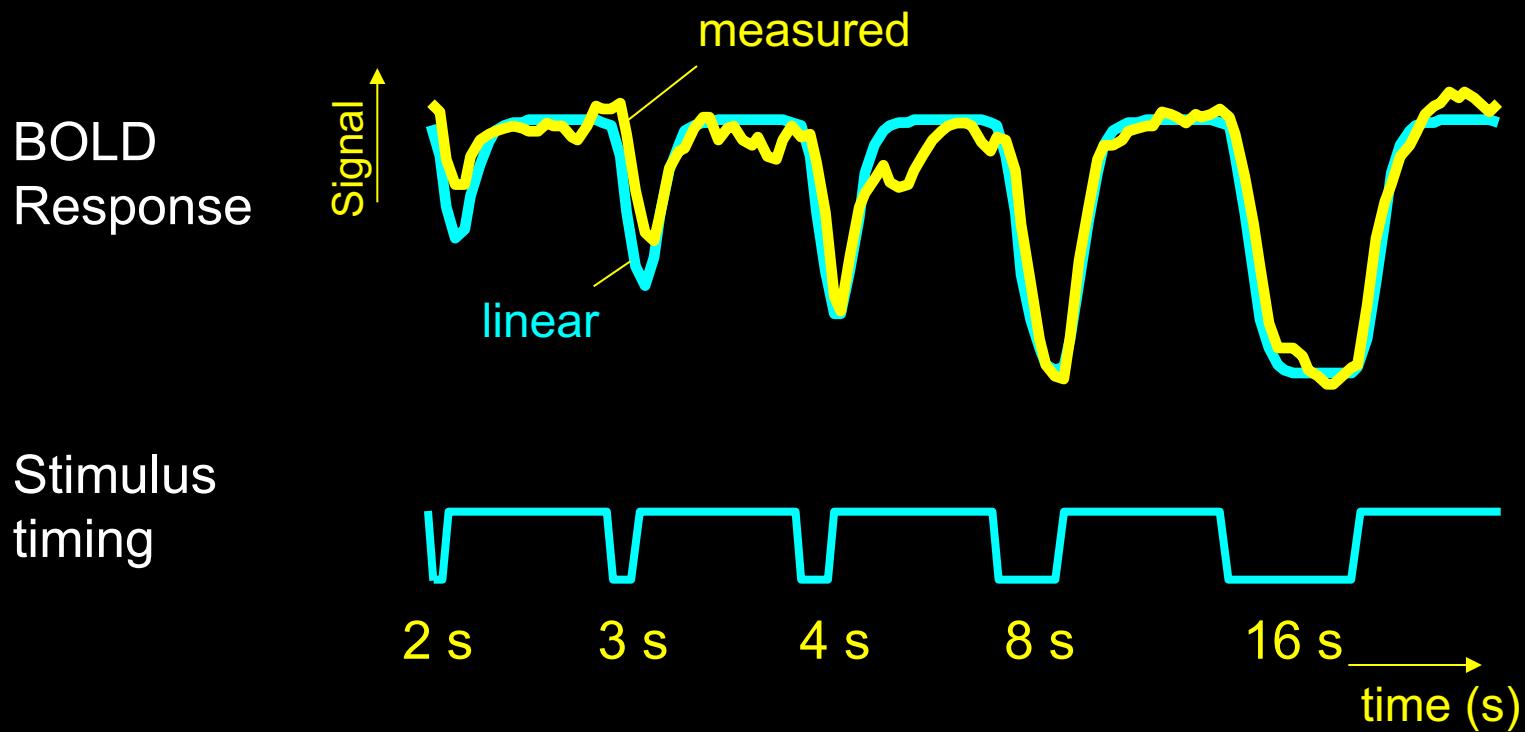
Magnitude



Latency



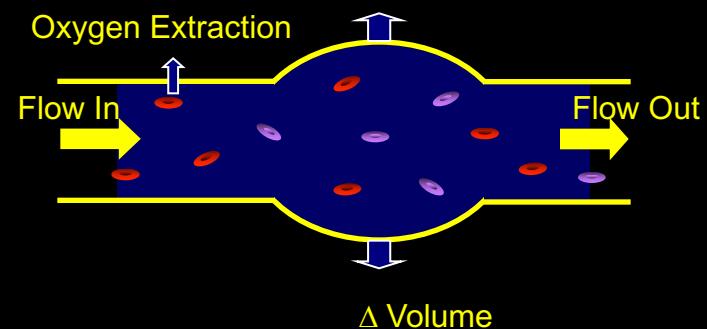
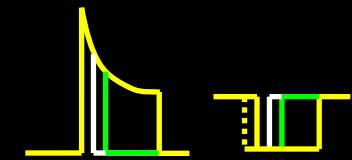
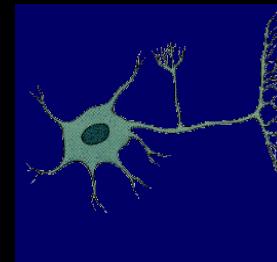
# Different stimulus “OFF” periods



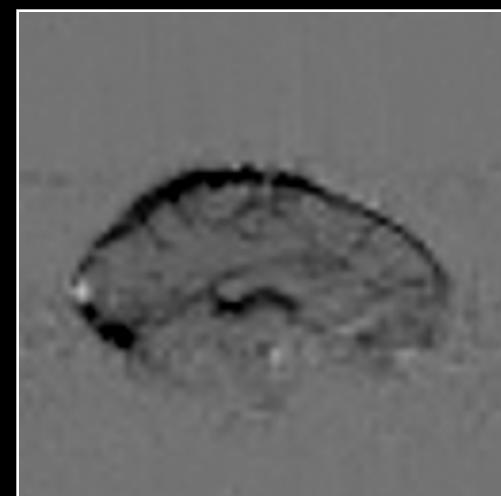
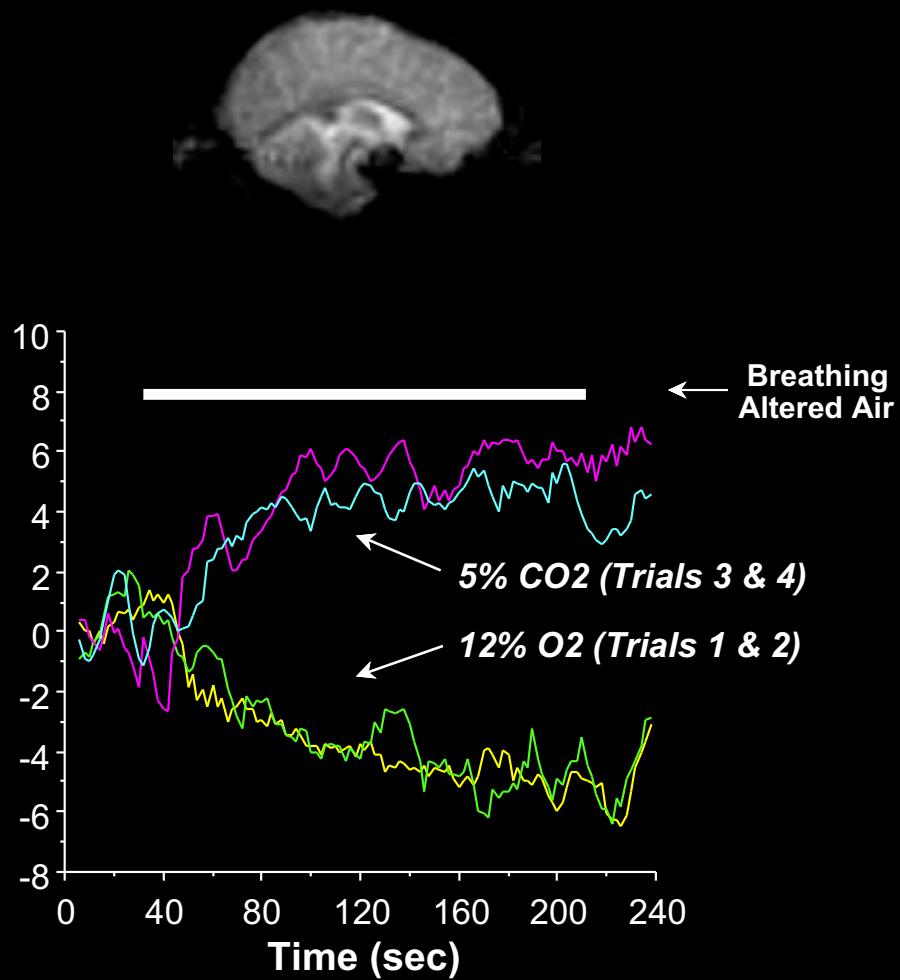
*Brief stimulus OFF periods produce smaller decreases than expected*

# Sources of this Nonlinearity

- Neuronal
- Hemodynamic
  - Oxygen extraction
  - Blood volume dynamics

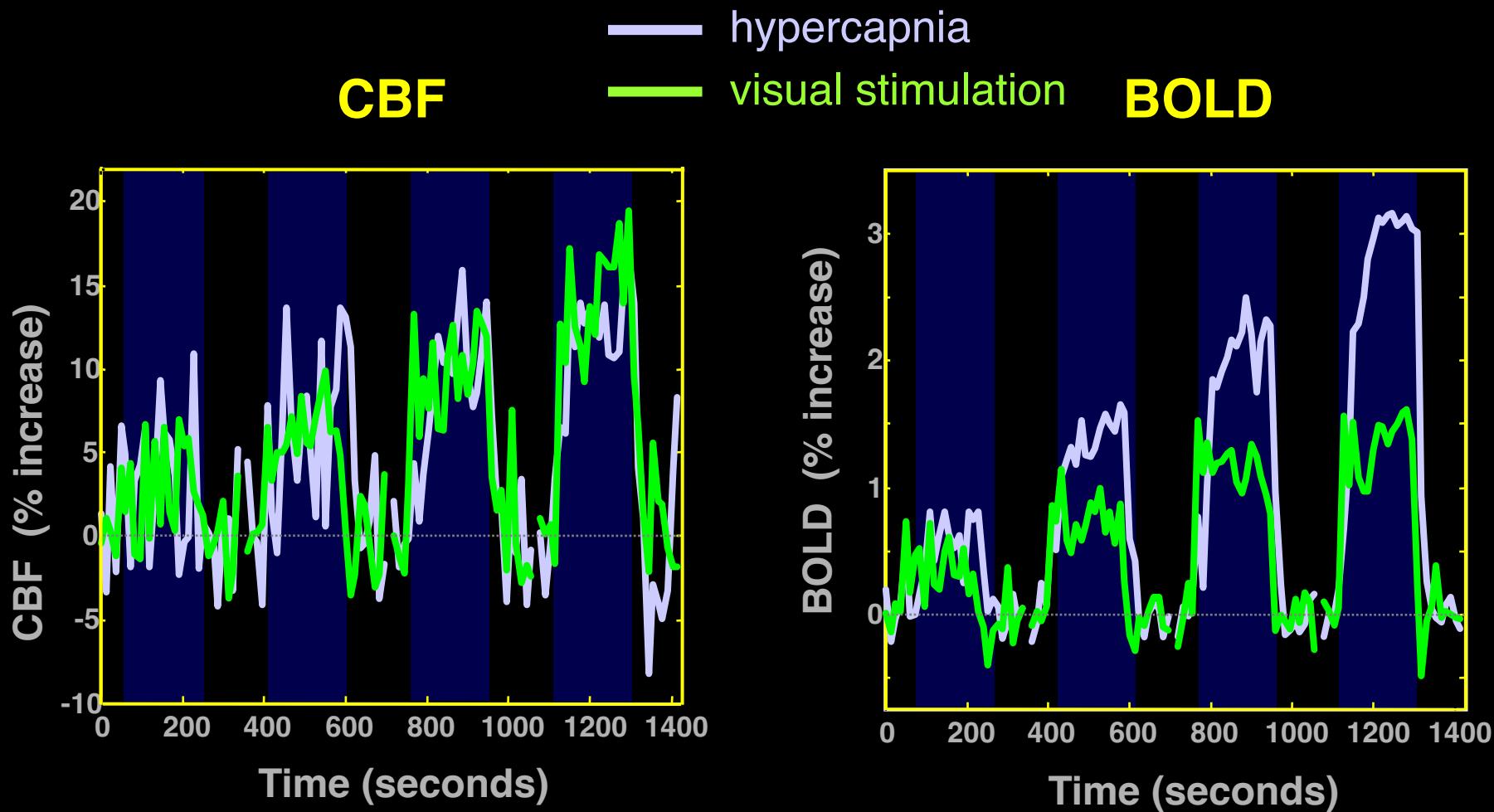


**5% CO<sub>2</sub>**



**12% O<sub>2</sub>**

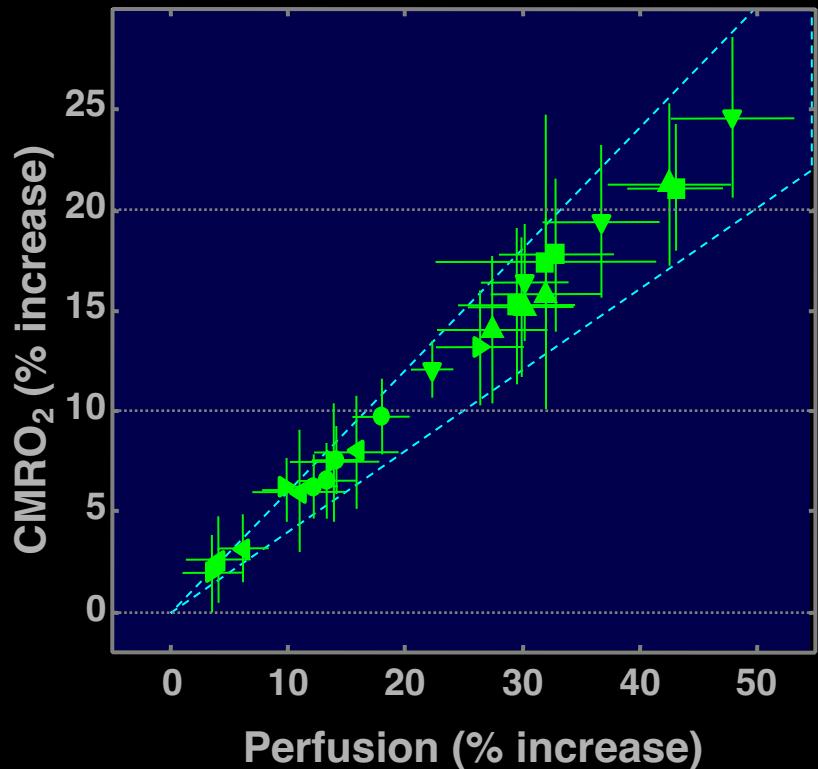
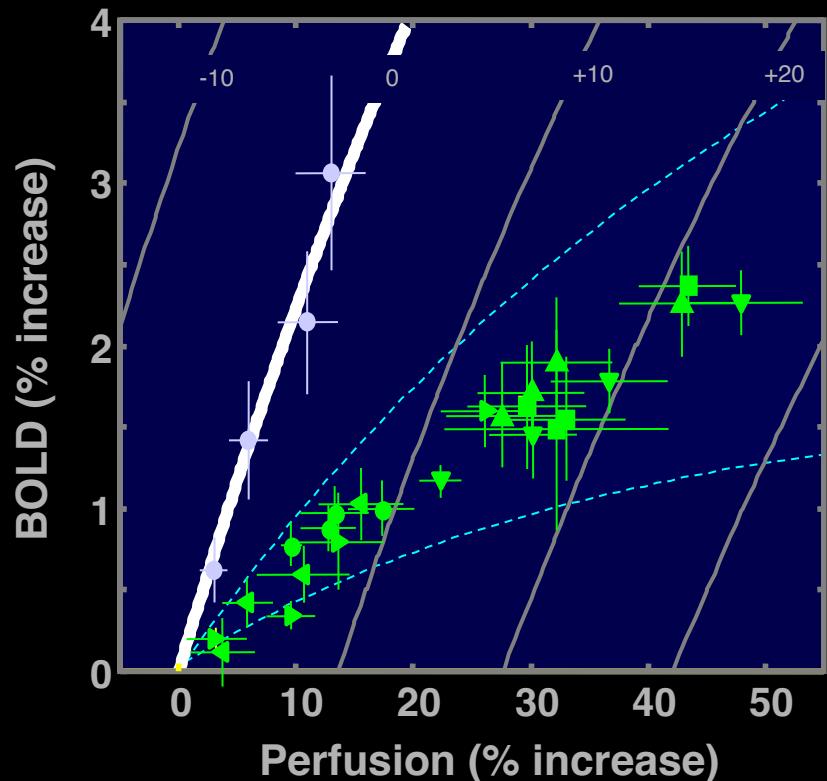
# CMRO<sub>2</sub>-related BOLD signal deficit:



Simultaneous Perfusion and BOLD imaging  
during graded visual activation and hypercapnia

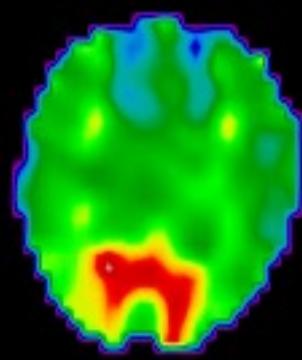
N=12

# CBF-CMRO<sub>2</sub> coupling

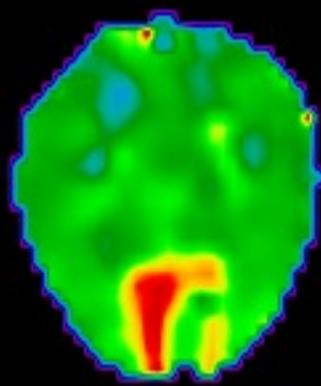


**Characterizing Activation-induced CMRO<sub>2</sub> changes using calibration with hypercapnia**

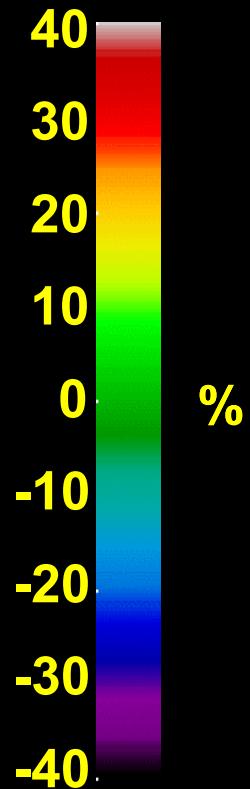
# Computed CMRO<sub>2</sub> changes



**Subject 1**



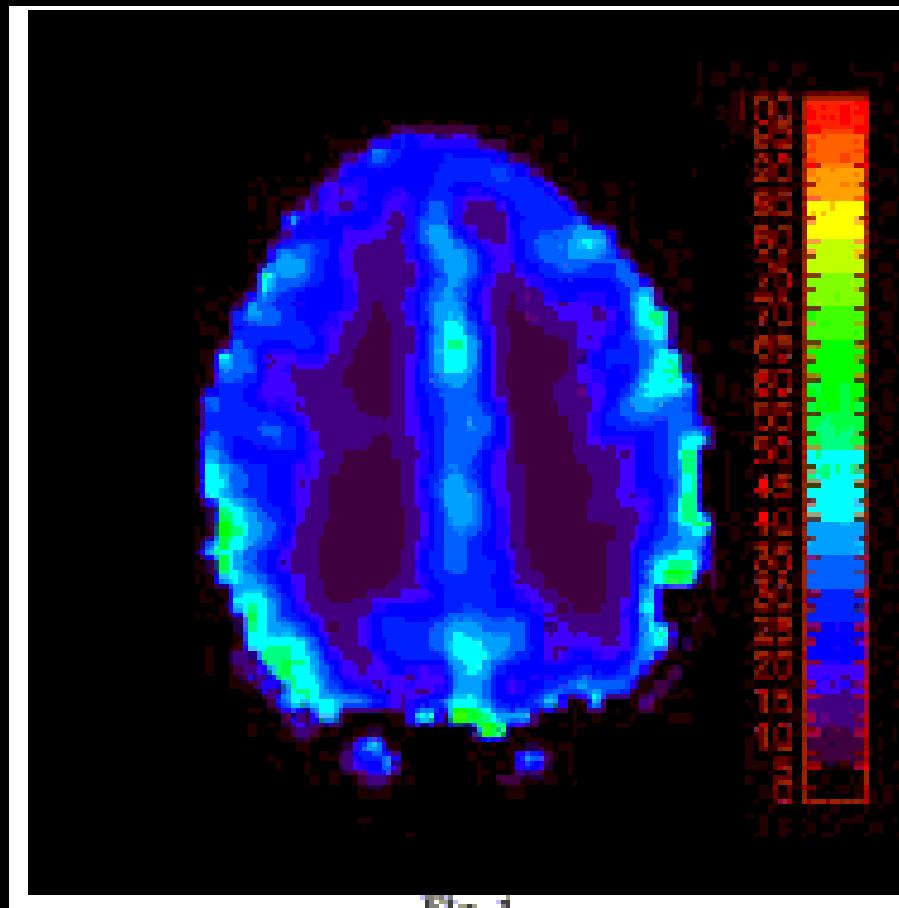
**Subject 2**



# Quantitative Measurements of Cerebral Metabolic Rate of Oxygen (CMRO<sub>2</sub>) Using MRI: A Volunteer Study

Honeyan AN<sup>1</sup>, Weili LIN<sup>2</sup>, Azim CELIK<sup>3</sup>, Yuesh Z. LEE<sup>4</sup>

<sup>1</sup>Washington University, 600 Airport Road, Chapel Hill, NC USA; <sup>2</sup>UNC-Chapel Hill, Department of Radiology, CB#7515, Chapel Hill, NC USA; <sup>3</sup>GE Medical Systems; <sup>4</sup>UNC-Chapel Hill, ;



# Neuronal Activation Input Strategies

1. Block Design

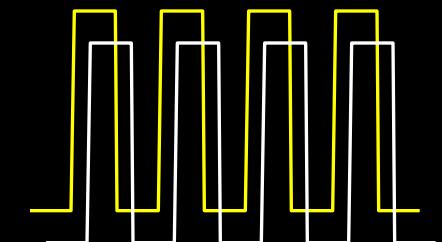
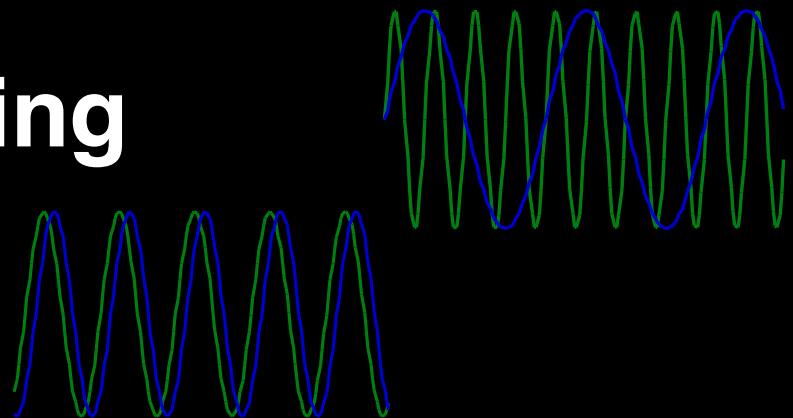
2. Frequency Encoding

3. Phase Encoding

4. Single Event

5. Orthogonal Block Design

6. Free Behavior Design.

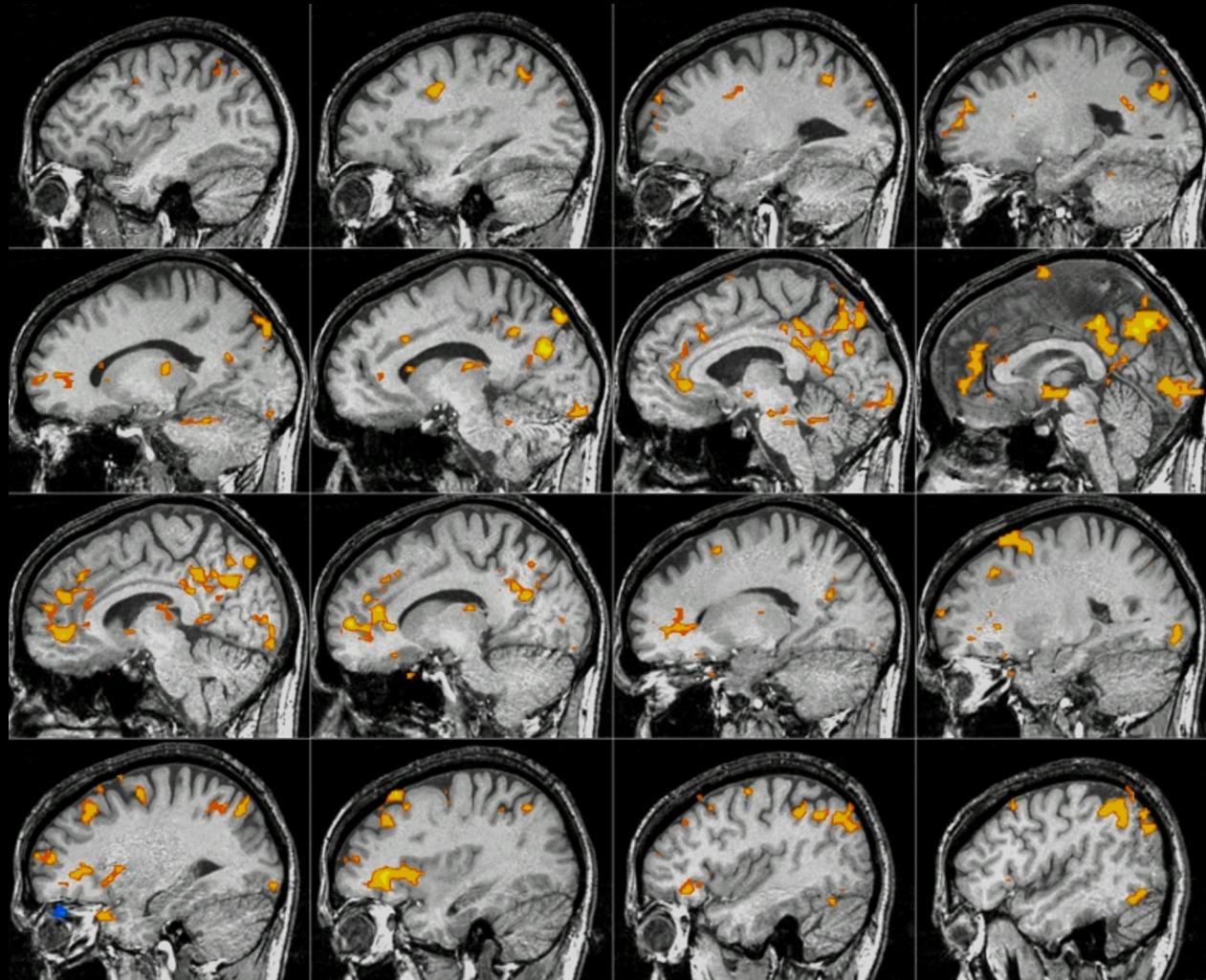


# Free Behavior Design

Use a continuous measure as a reference function:

- Task performance
- Skin Conductance
- Heart, respiration rate..
- Eye position
- EEG

# Brain activity correlated with SCR during “Rest”



# Pushing the Envelope...

1. Temporal Resolution
2. Spatial Resolution
3. Sensitivity and Noise
4. Information Content
5. Implementation

# Motion

Recognize?

- Edge effects
- Shorter signal change latencies
- Unusually high signal changes
- External measuring devices

Correct?

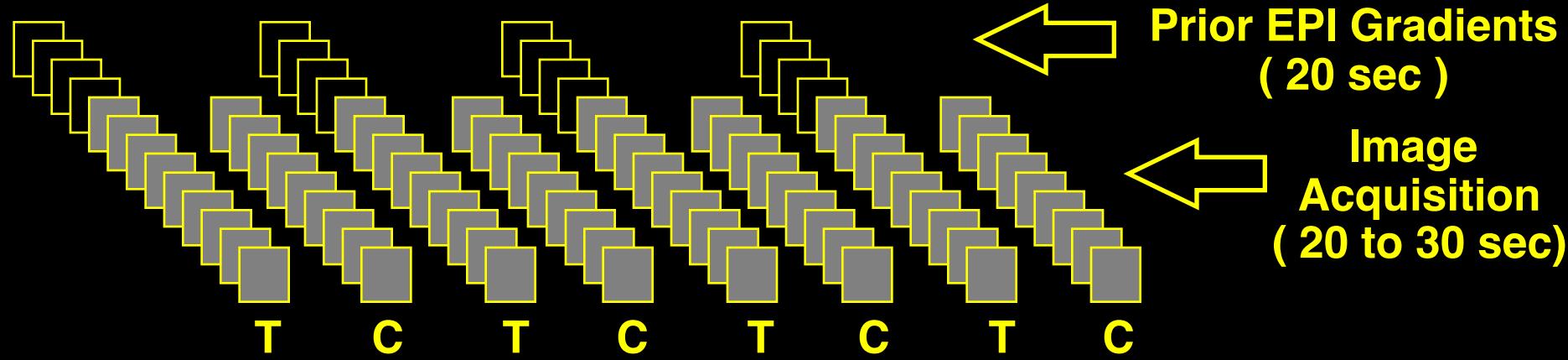
- Image registration algorithms
- Orthogonalize to motion-related function (*cardiac, respiration, movement*)
- Navigator echo for k-space alignment  
*(for multishot techniques)*
- Re-do scan

Bypass?

- Paradigm timing strategies..
- Gating (with T1-correction)

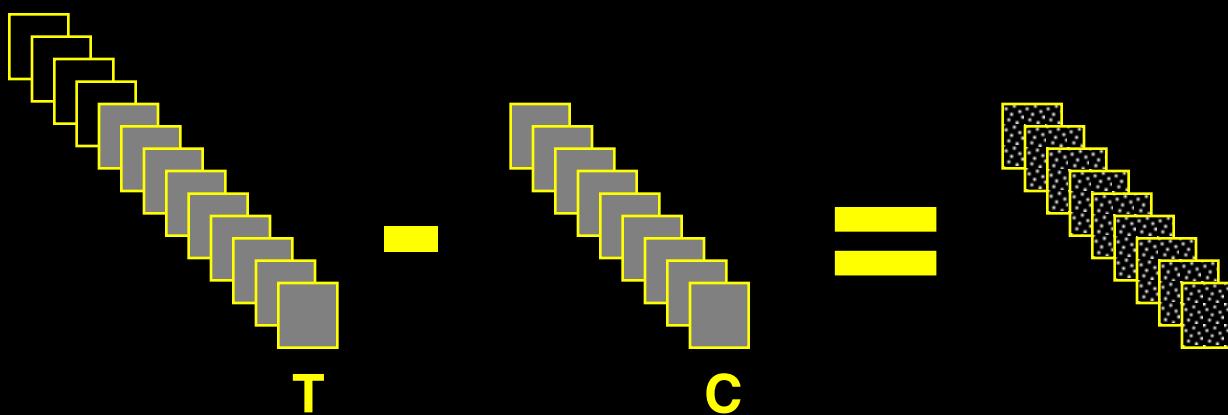
Suppress?

- Flatten image contrast
- Physical restraint
- Averaging, smoothing



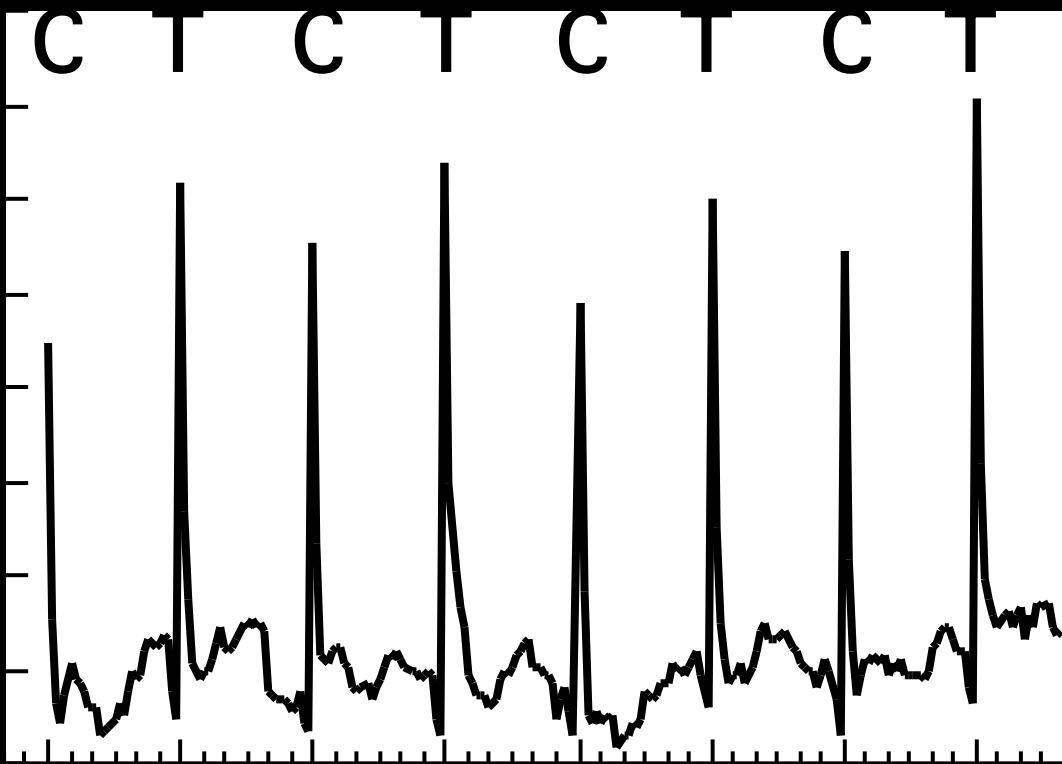
Prior EPI Gradients  
( 20 sec )

Image  
Acquisition  
( 20 to 30 sec )

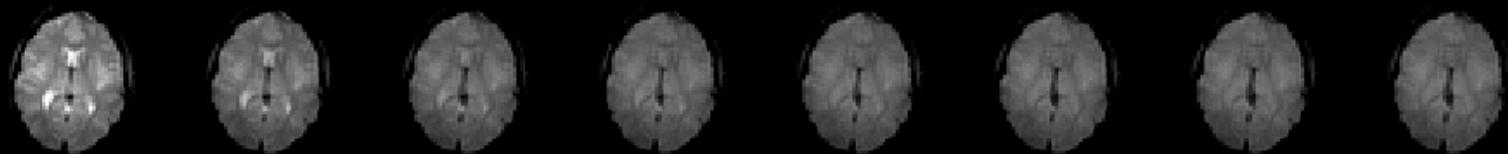


Average Time Series

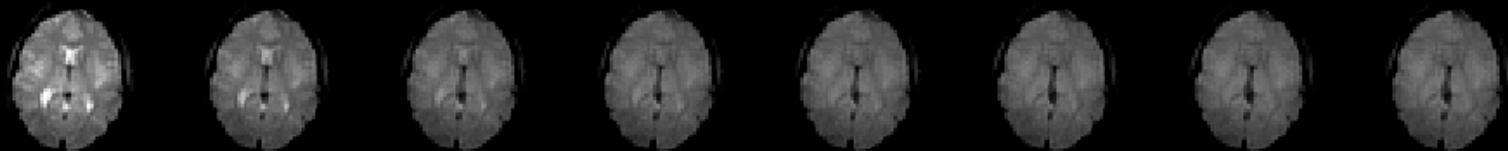
Difference Time Series



**a.**



**b.**



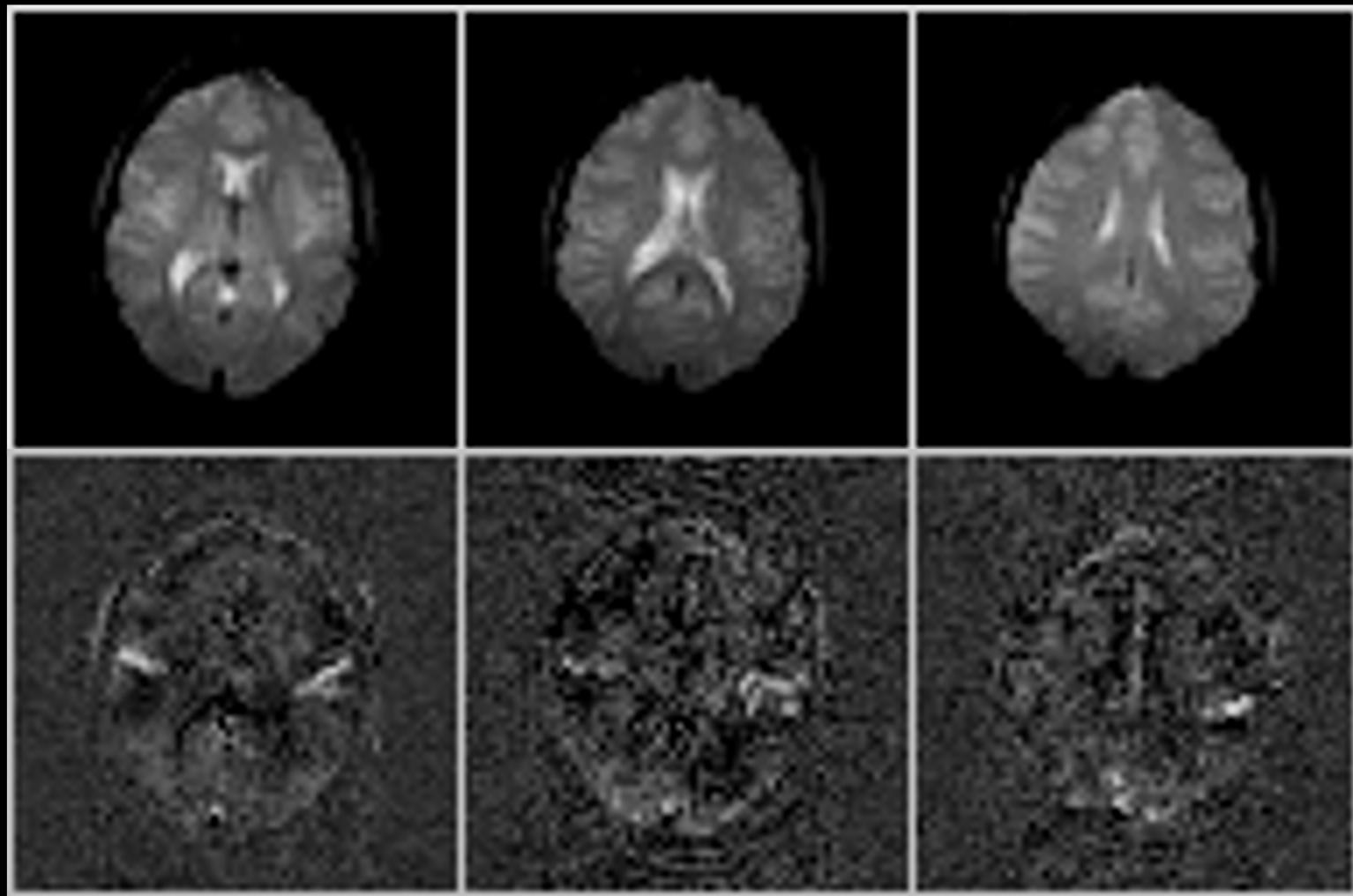
**c.**



0      1      2      3      4      5      6      7

**Time (sec)**



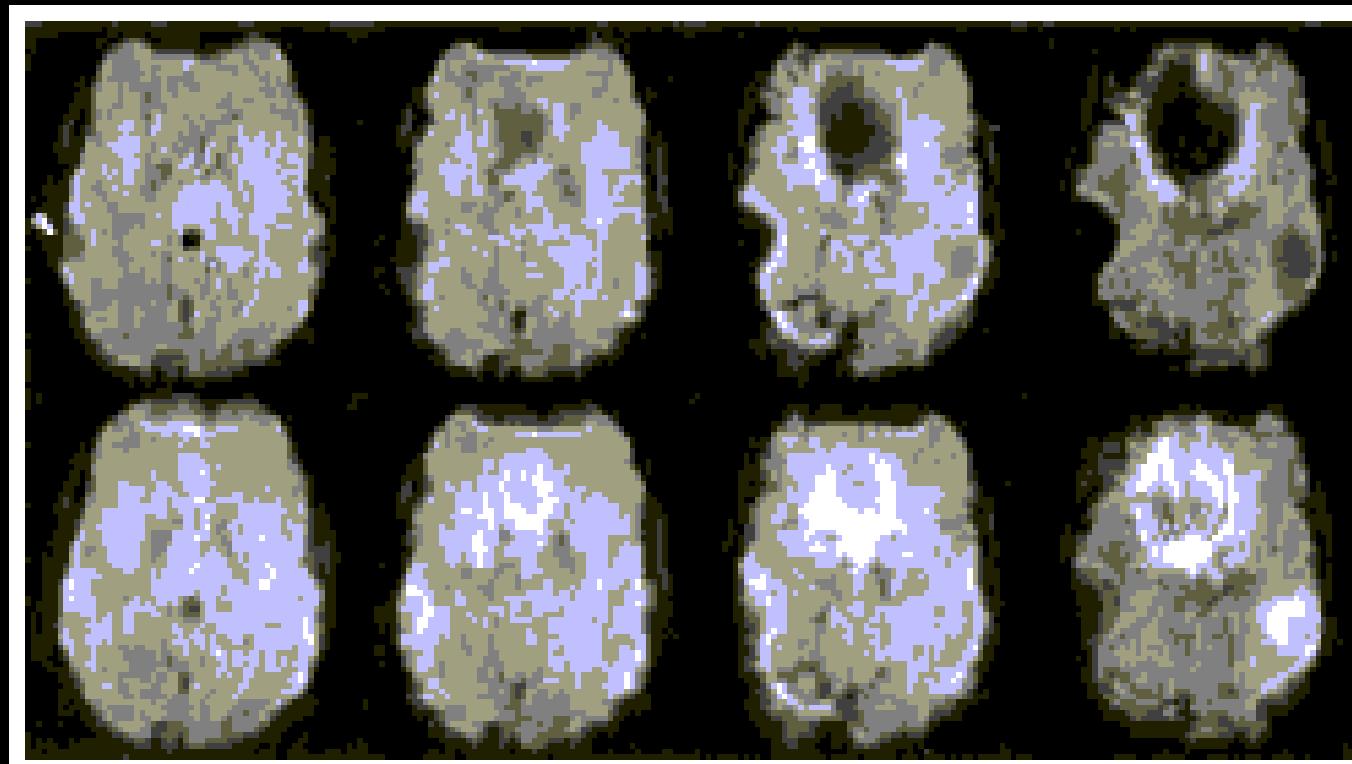


# How to deal with Scanner Noise?

- Clustered volume acquisition  
Talavage et al.
- Silent sequences

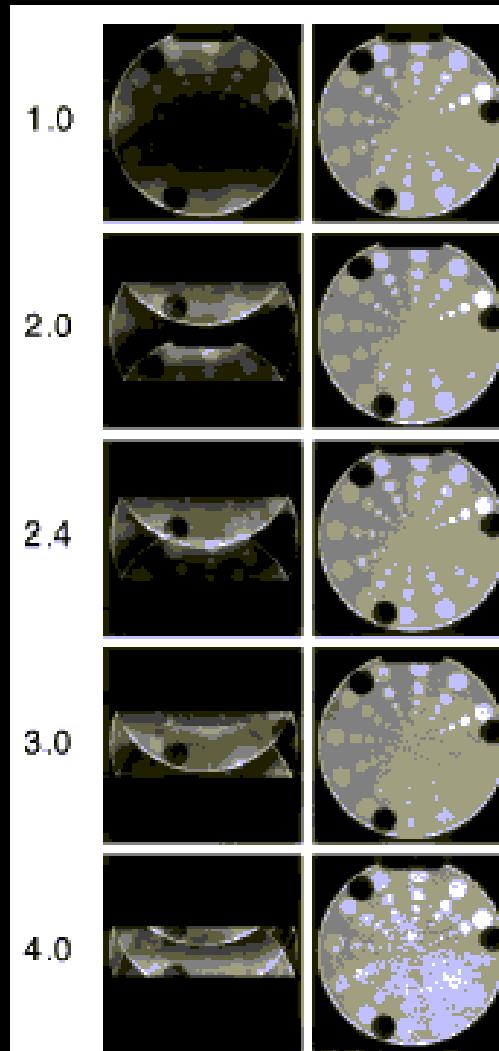
## 3D z-Shim Method for Reduction of Susceptibility Effects in BOLD fMRI

Gary H. Glover\*



# SENSE: Sensitivity Encoding for Fast MRI

Klaas P. Pruessmann, Markus Weiger, Markus B. Scheidegger, and Peter Boesiger\*



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August, 2000