

# Time-Frequency analysis of biophysical time series

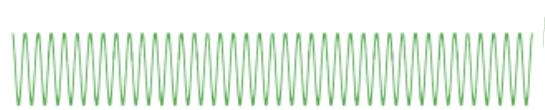
*Nov 18<sup>th</sup> 2010, 12<sup>th</sup> EEGLAB workshop*

Arnaud Delorme

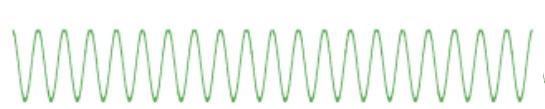
SCCN, UCSD  
CERCO, CNRS

# Frequency analysis

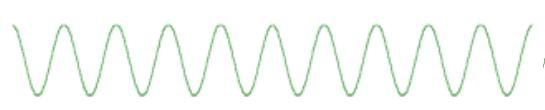
synchronicity of cell excitation determines amplitude and rhythm of the EEG signal



30-60 Hz Gamma



18-21 Hz Beta



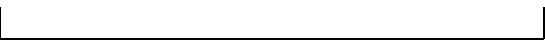
9-11 Hz Alpha



4-7 Hz Theta

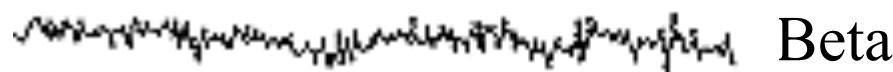


0.5-2 Hz Delta



1 second

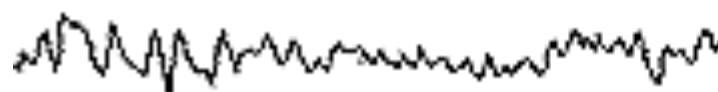
# Frequency analysis



Beta



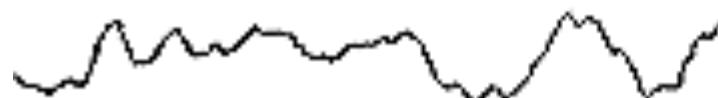
Alpha



Theta

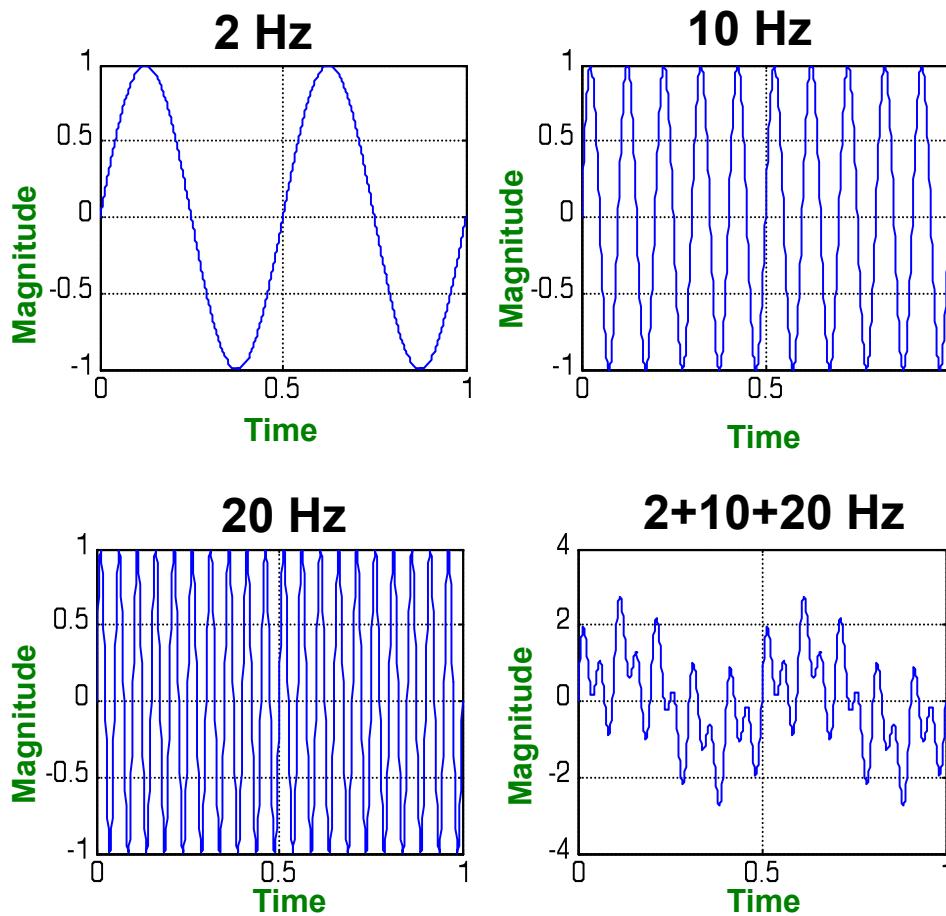


Delta



Low Delta

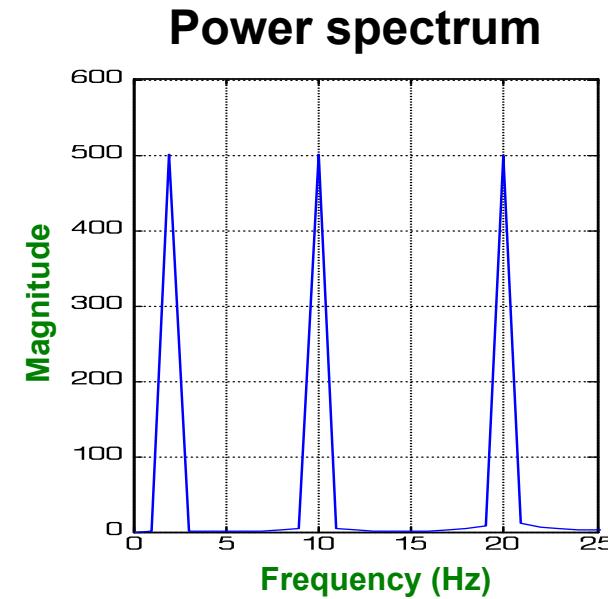
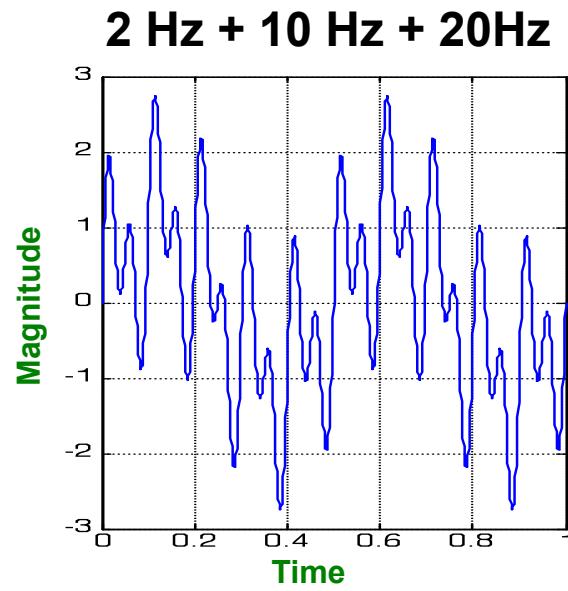
# Stationary signals



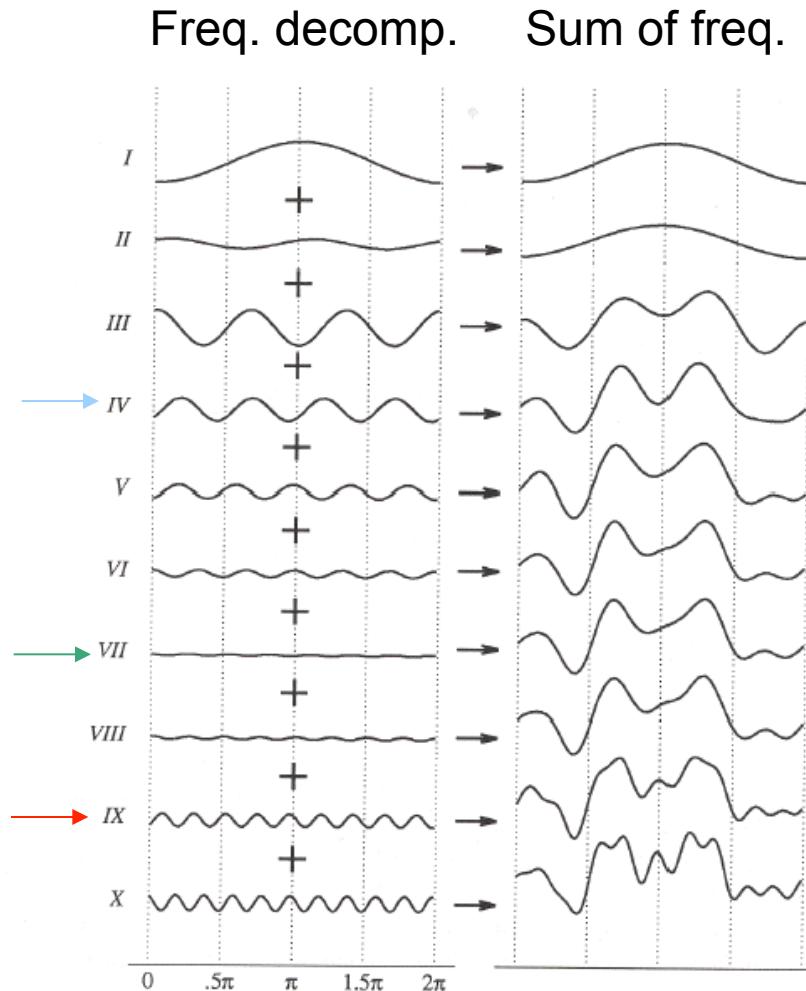
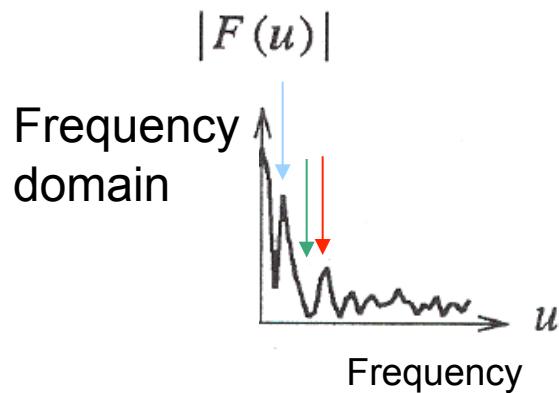
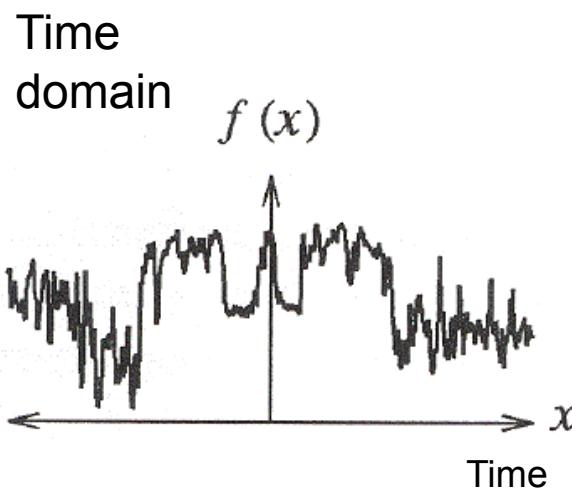
Slide courtesy of Petros Xanthopoulos, Univ. of Florida

# Stationary signal

Stationary



By looking at the Power spectrum of the signal we can recognize three frequency Components (at 2,10,20Hz respectively).



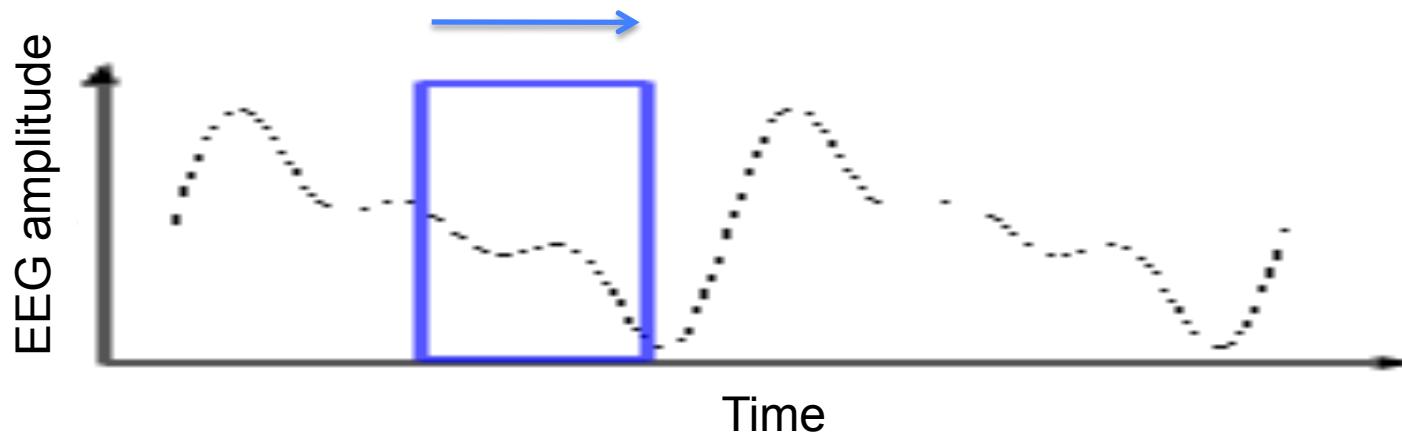
Forward transform

$$F(u) = \int_{-\infty}^{+\infty} f(x)e^{-2\pi iux} dx$$

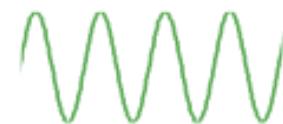
Inverse transform

$$f(x) = \int_{-\infty}^{+\infty} F(u)e^{2\pi iux} du$$

Figure, courtesy of Ravi Ramamoorthi & Wolberg



Sinusoid



Gaussian

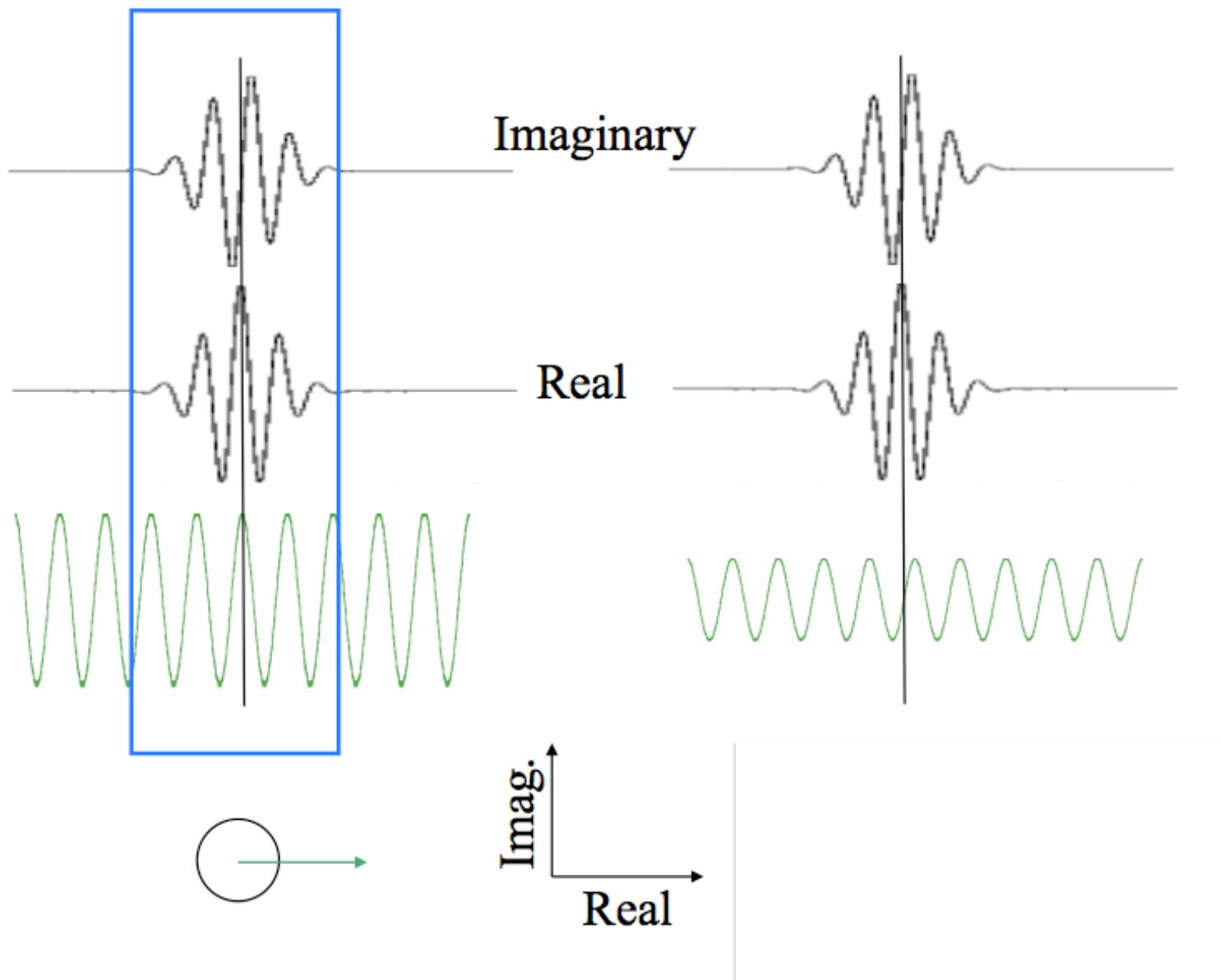


Tapered  
sinusoid

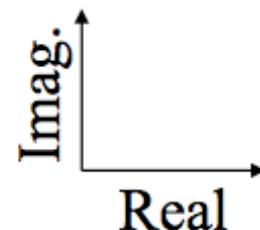
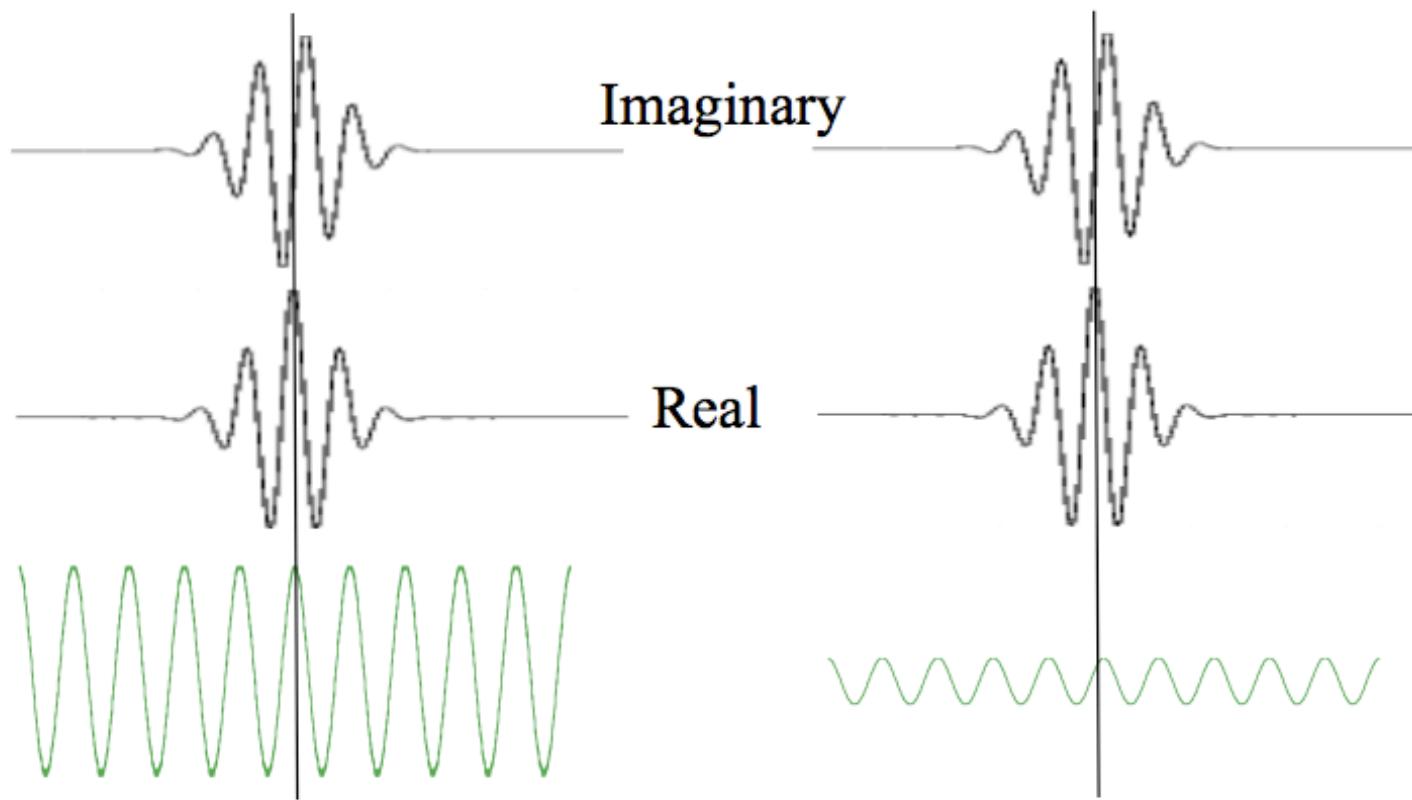


Performing Fourier transform by using  
a time moving  
window

# Spectral phase and amplitude



# Spectral phase and amplitude



# Discrete Fourier Transform function

```
function X = dft(x)
```

```
[N,M] = size(x);  
n = 0:N-1;
```

```
for k=n
```

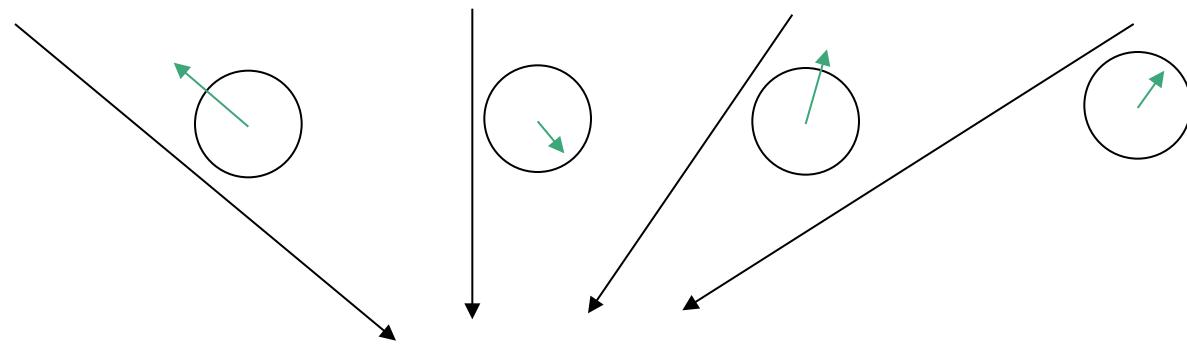
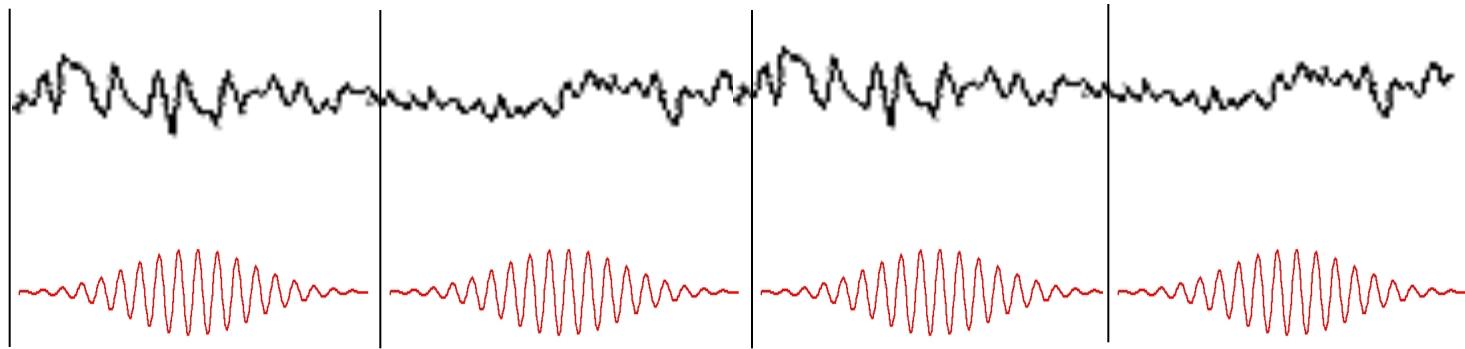
```
    X(k+1) = exp(-j*2*pi*k*n/N)*x;  
end
```

Loop on frequency

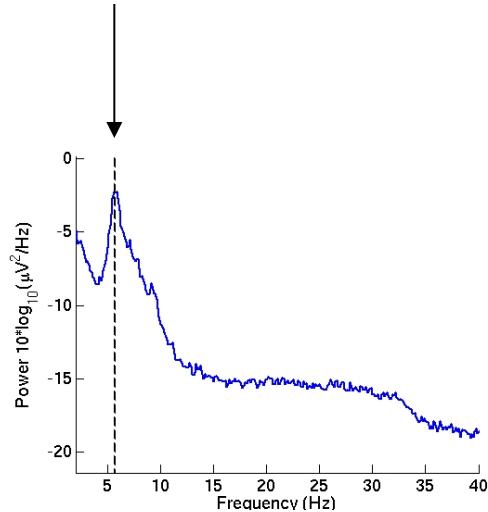
Multiply with signal

Imaginary part  
Sine component

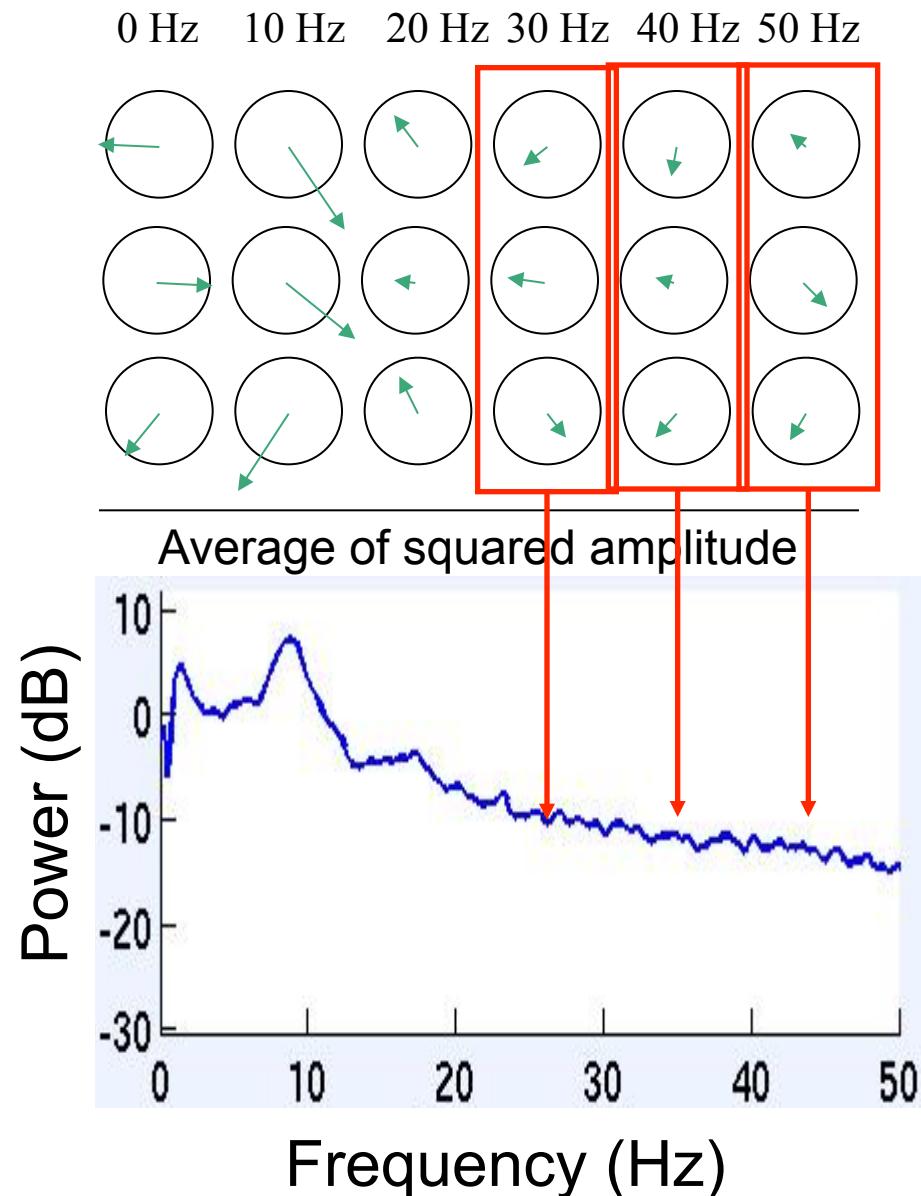
Real part  
Cosine component

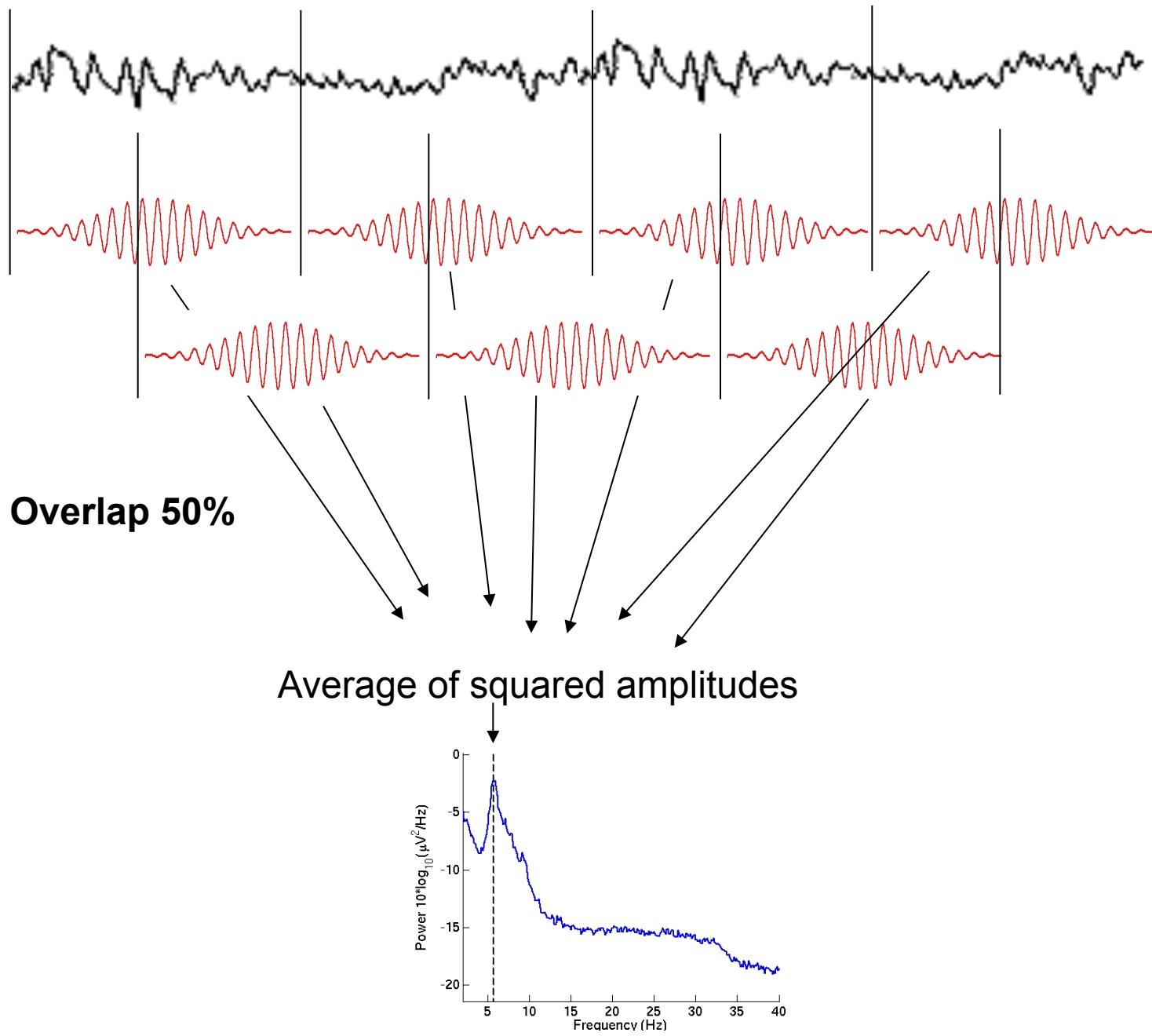


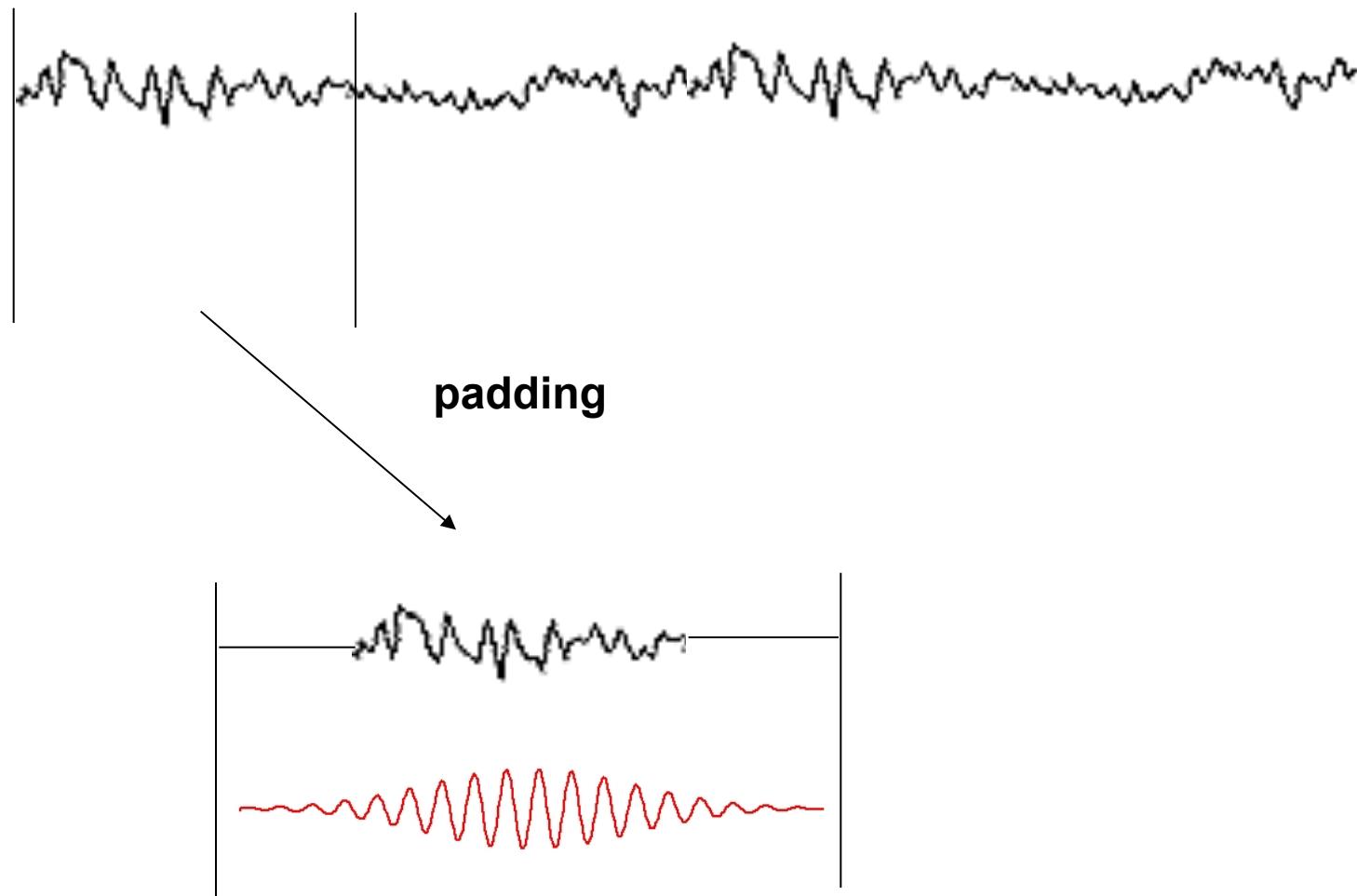
Average of squared absolute values



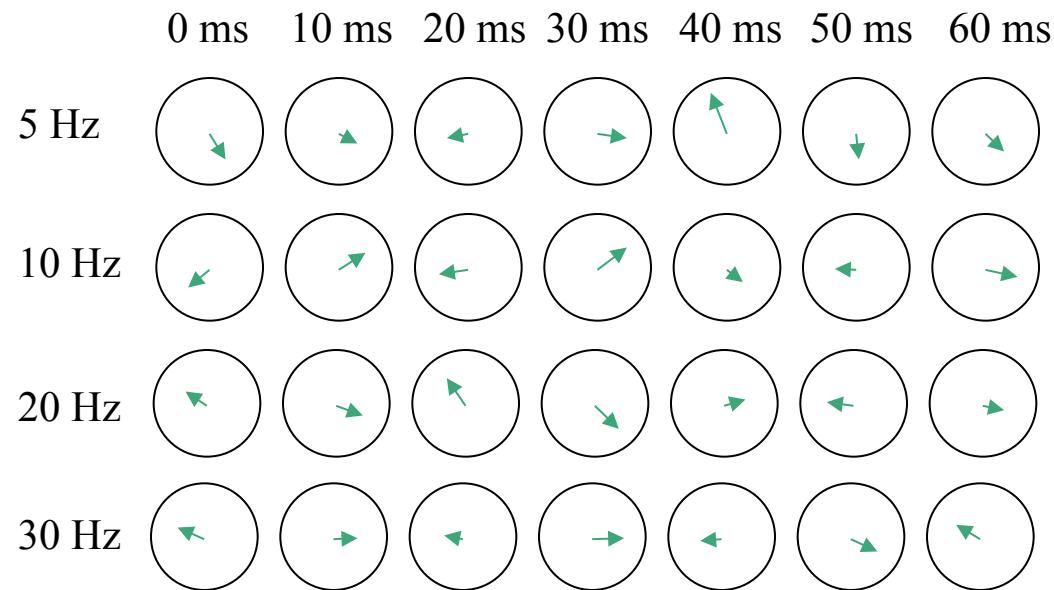
# Spectral power



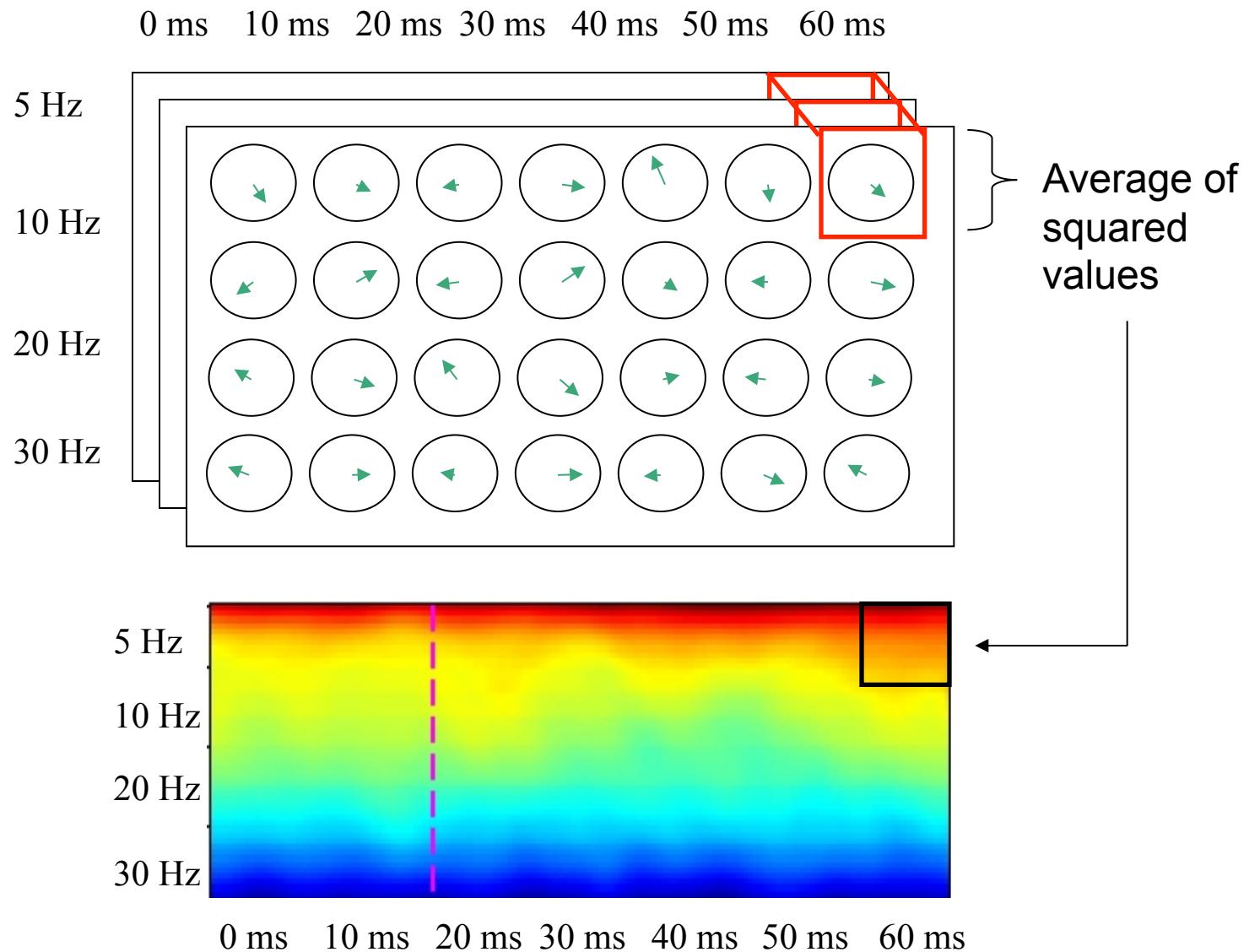




# Spectrogram or ERSP



# Spectrogram or ERSP



# Power spectrum and event-related spectral perturbation

$$ERS(f,t) = \frac{1}{n} \sum_{k=1}^n |F_k(f,t)|^2$$

↓

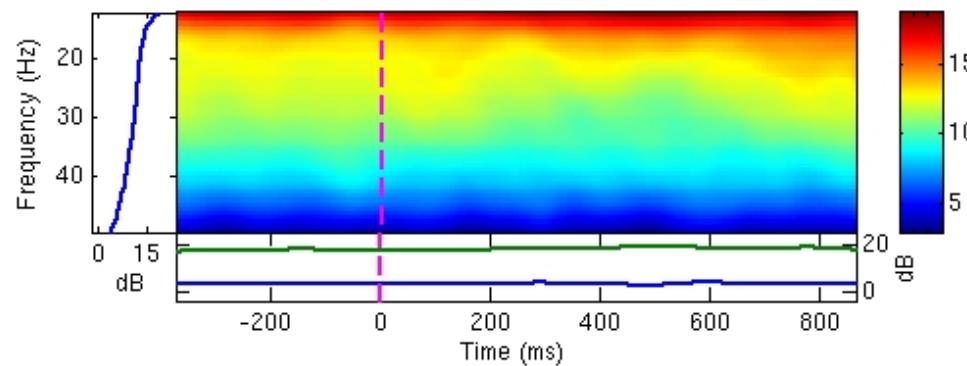
↑

Complex number

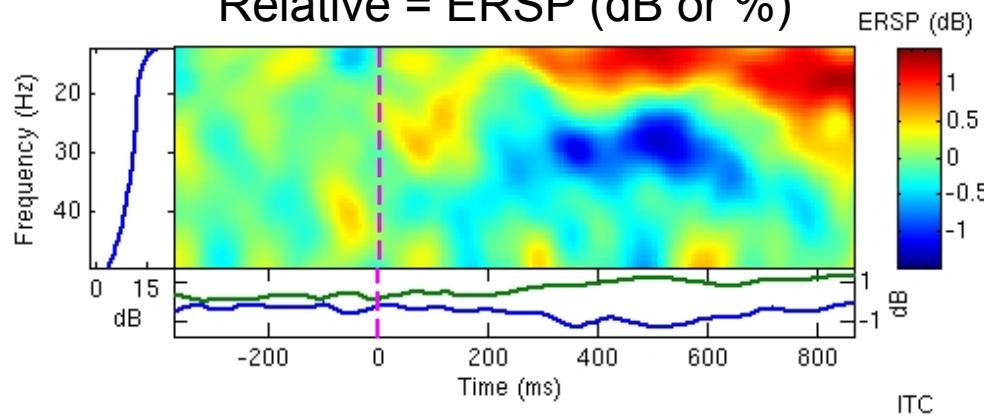
Scaled to dB  $10\log_{10}(ERSP)$

# Absolute versus relative power

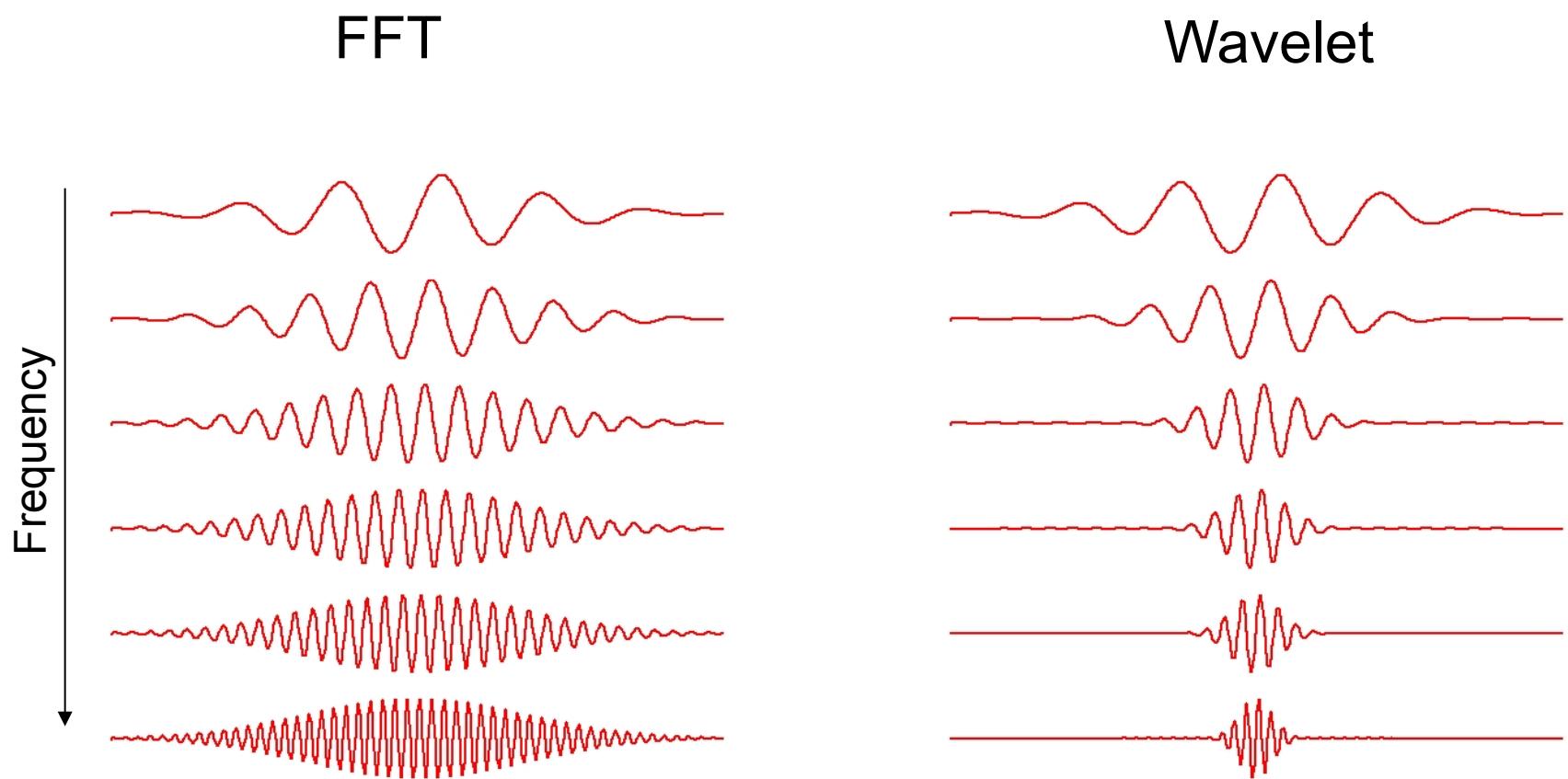
Absolute = ERS



Relative = ERSP (dB or %)

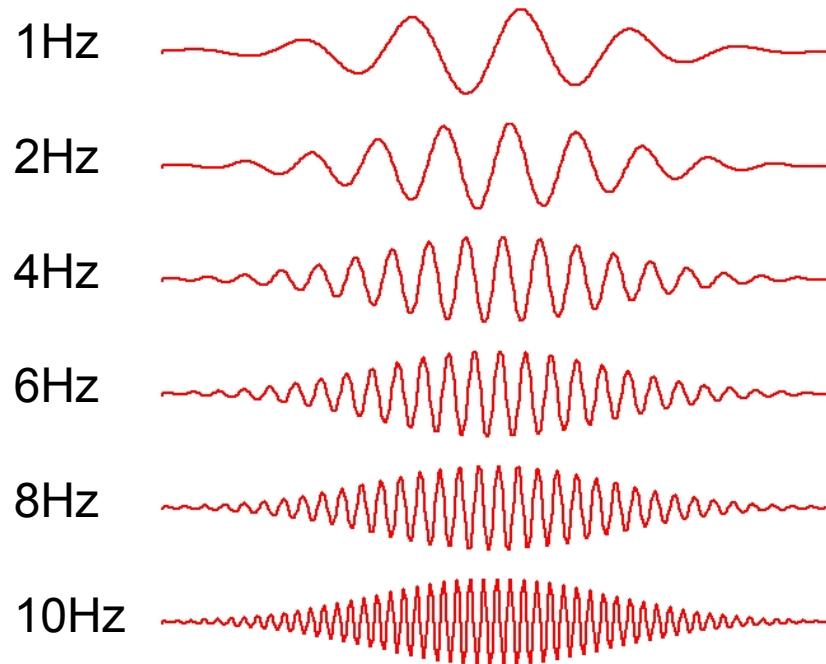


# Difference between FFT and wavelets

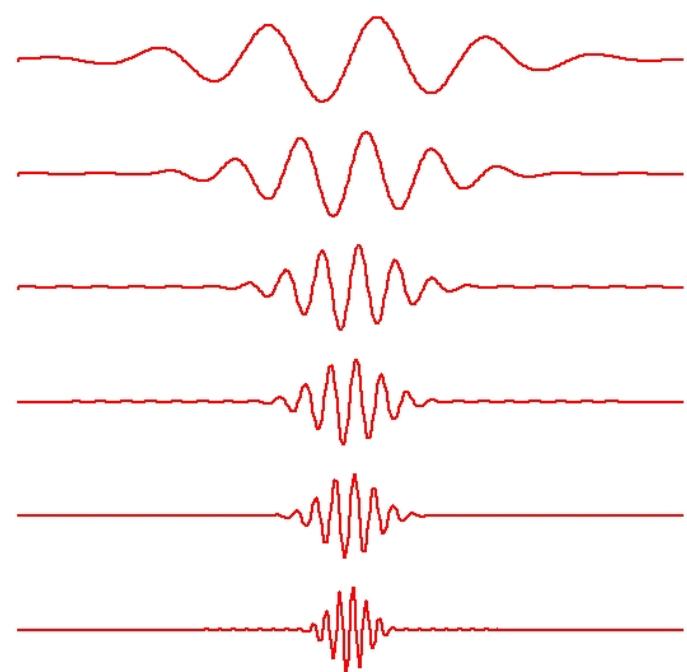


# Wavelets factor

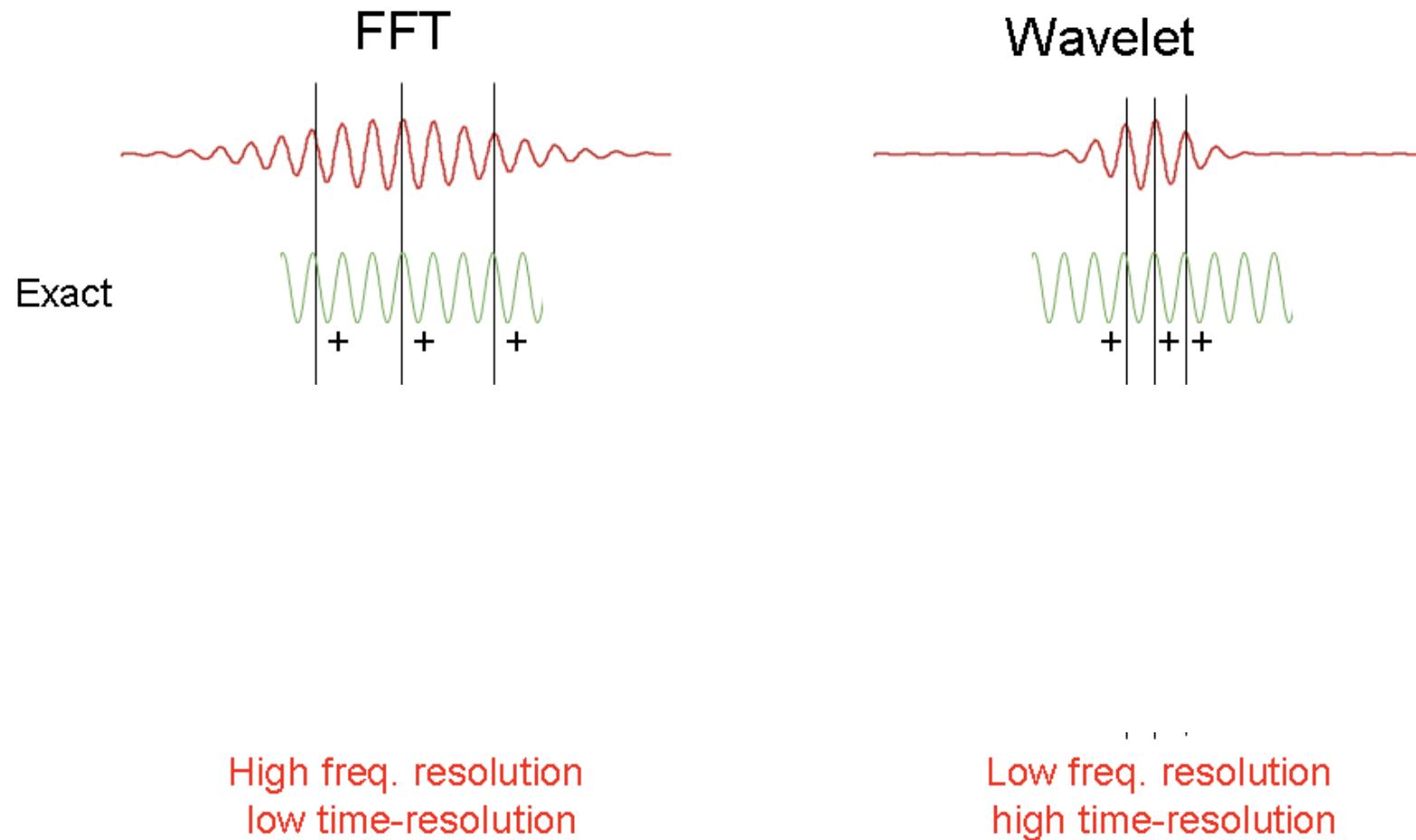
Wavelet (0)= FFT



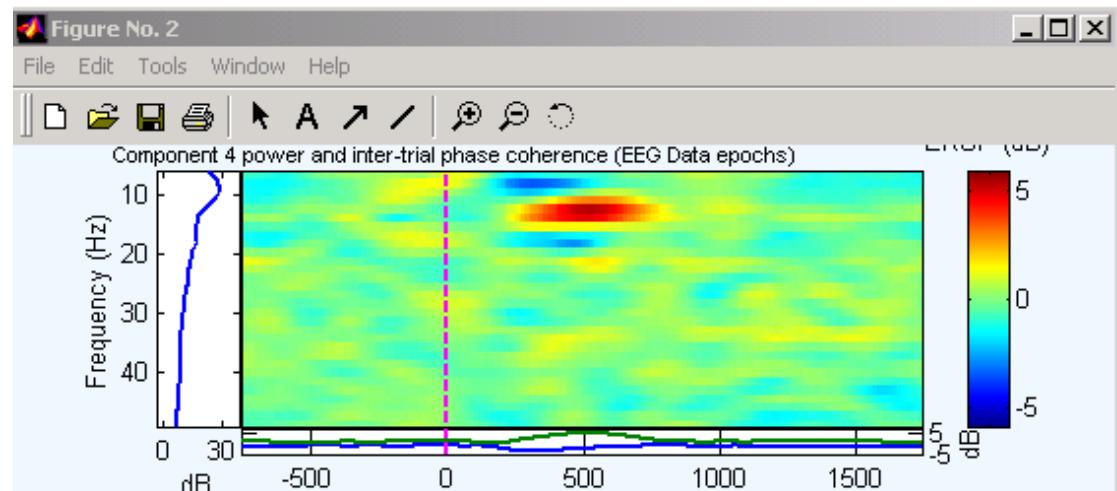
Wavelet (1)



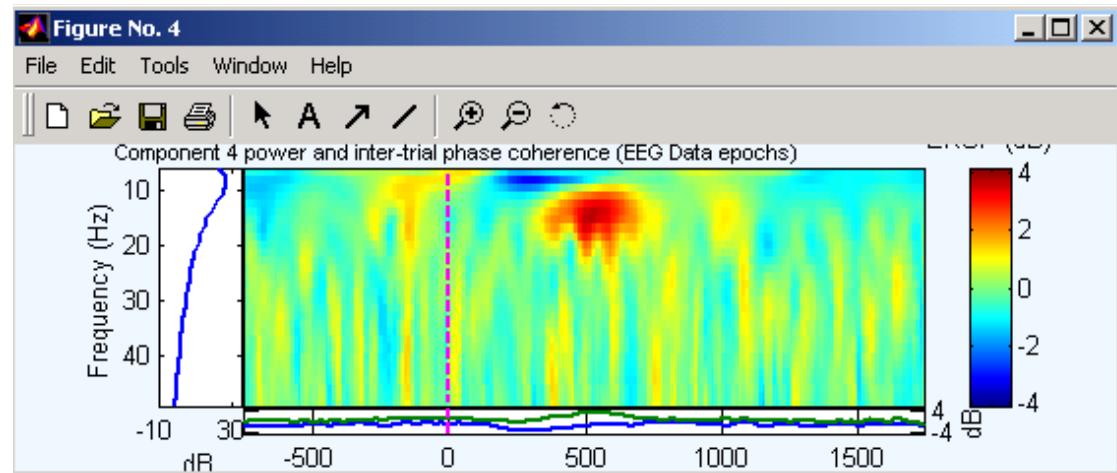
# Time-frequency resolution trade off



# FFT



# Pure wavelet



# The Uncertainty Principle

A signal cannot be localized arbitrarily well both in time/position and in frequency/momentum.

There exists a lower bound to the *Heisenberg's product:*

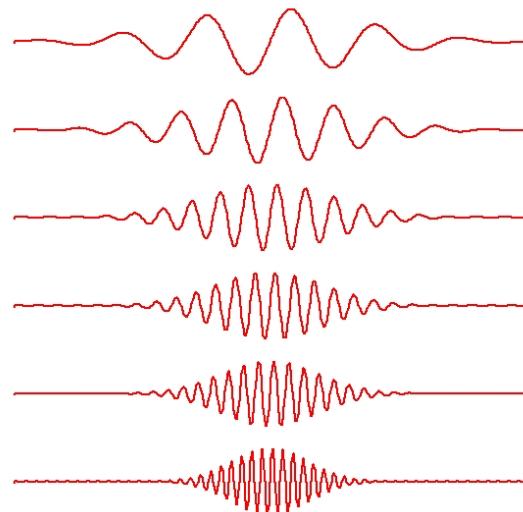
$$\Delta t \Delta f \geq 1/(4\pi)$$



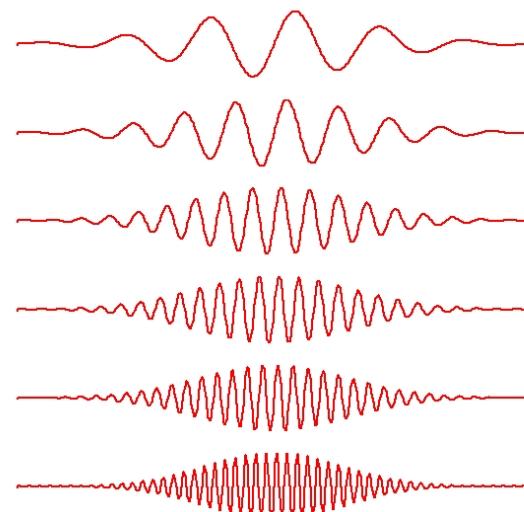
$$\Delta f = 1\text{Hz}, \Delta t = 80\text{ msec} \text{ or } \Delta f = 2\text{Hz}, \Delta t = 40\text{ msec}$$

# Modified wavelets

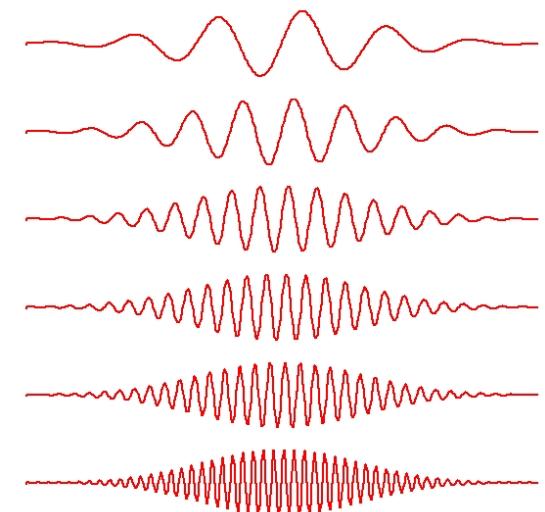
Wavelet (0.8)



Wavelet (0.5)

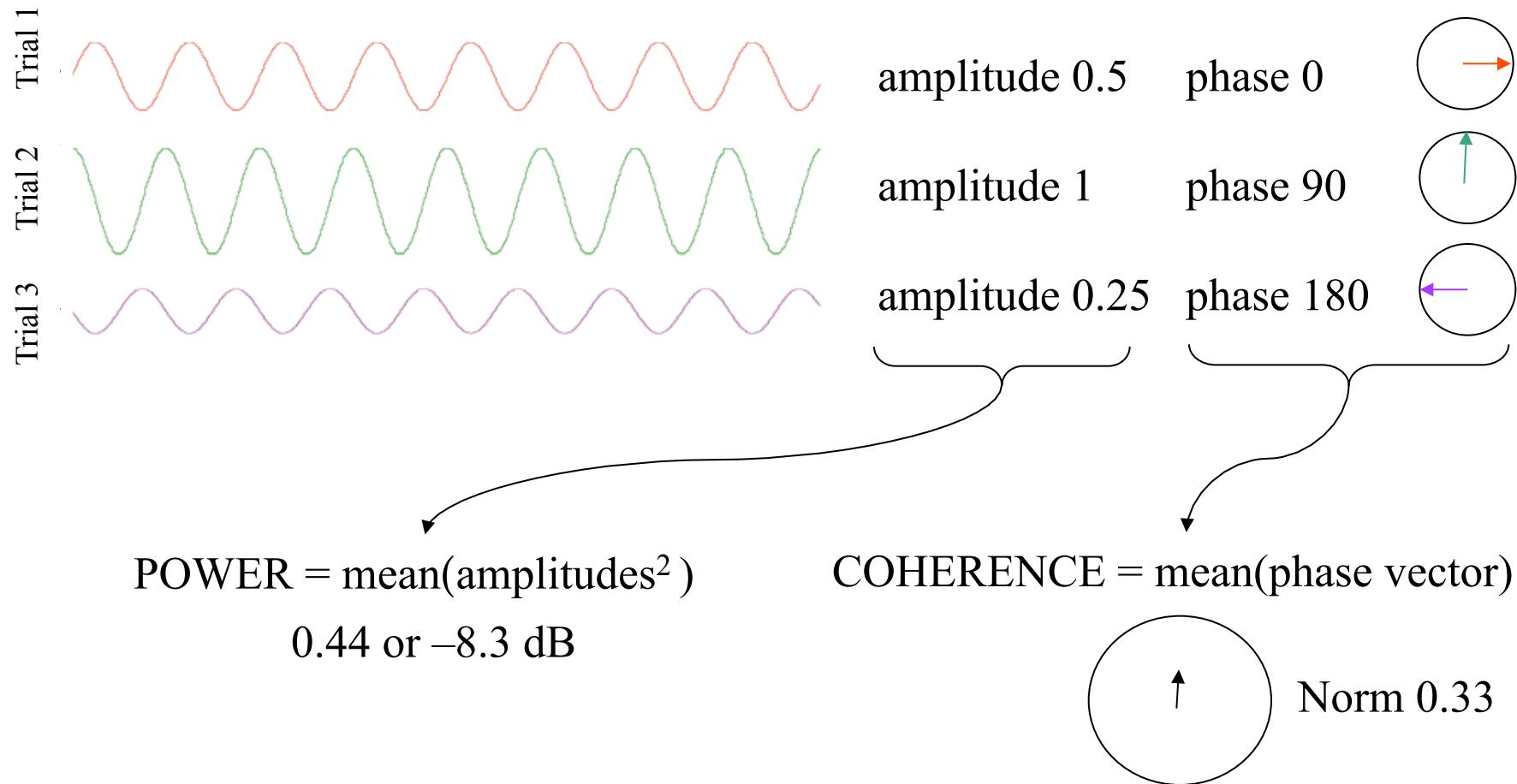


Wavelet (0.2)

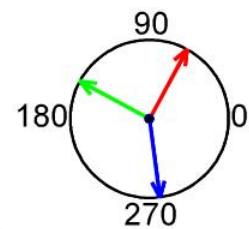
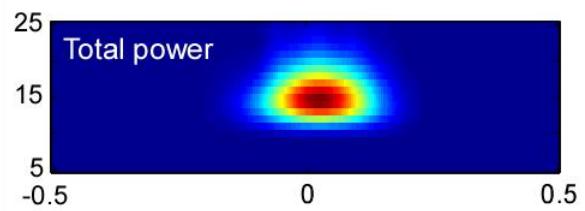
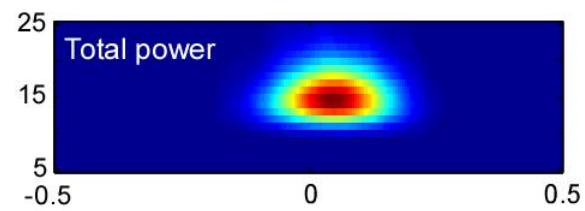
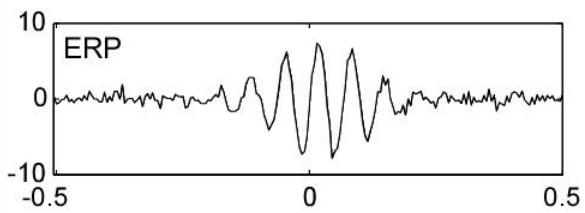
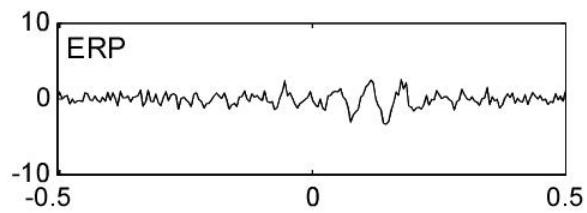
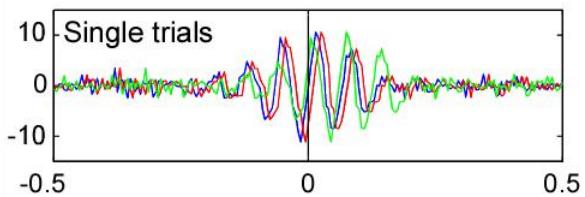
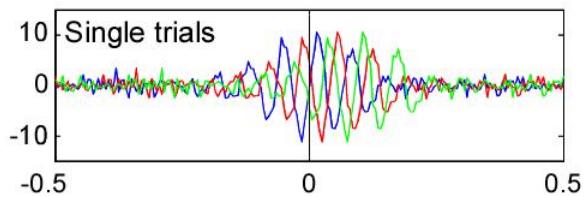


# Inter trial coherence

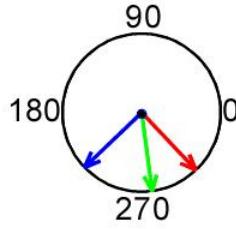
same time, different trials



## Intertrial Coherence (ITC)



ITC: .05



ITC: .80

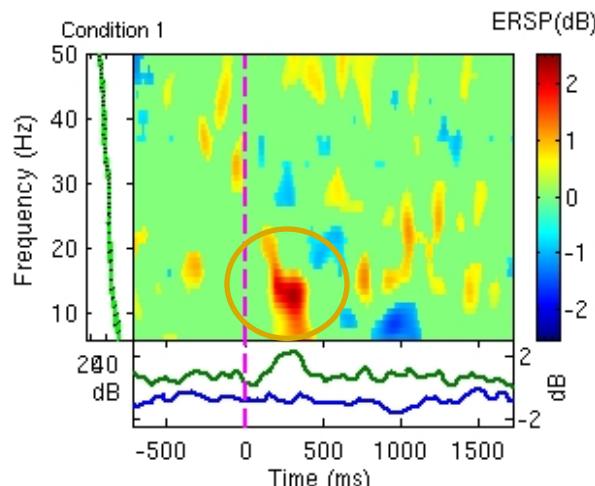
## Phase ITC

$$ITPC(f, t) = \frac{1}{n} \sum_{k=1}^n \frac{F_k(f, t)}{|F_k(f, t)|}$$

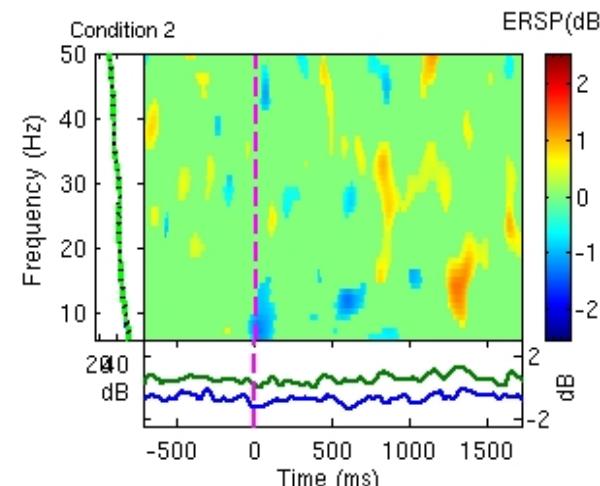
Normalized  
(no amplitude information)

# Power and inter trial coherence

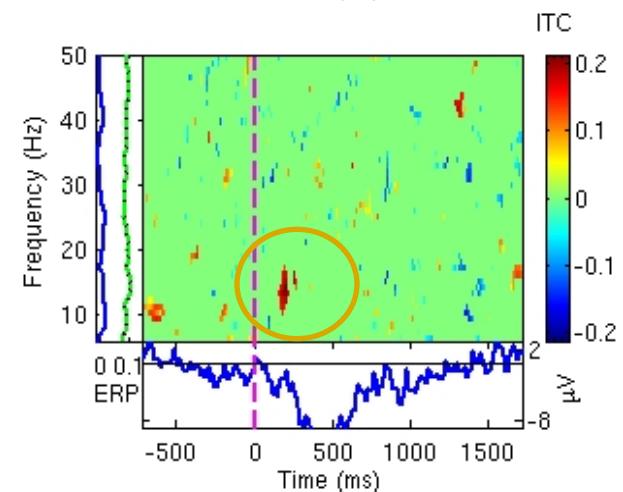
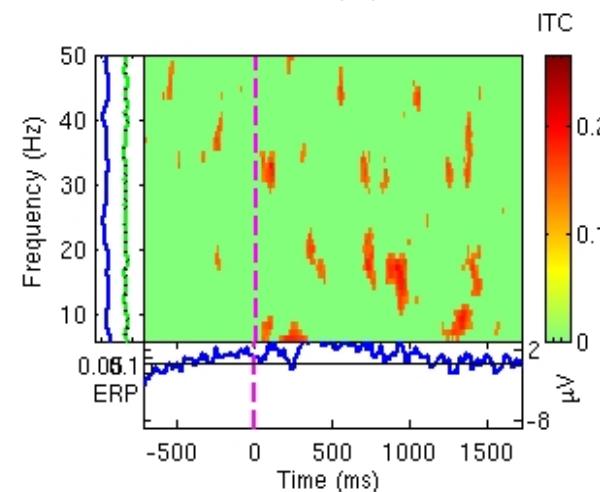
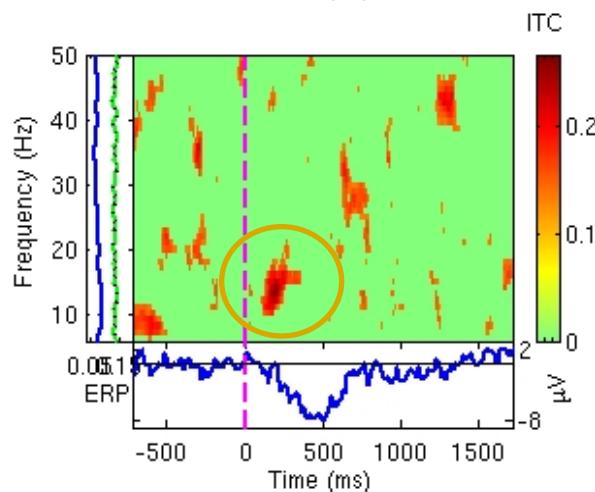
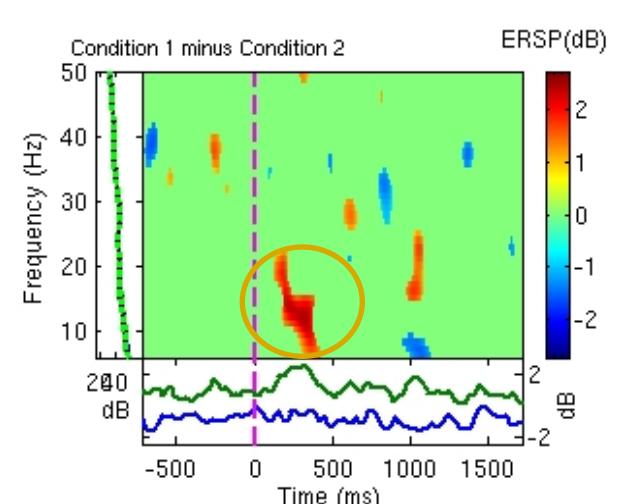
*Attend left-stim left*

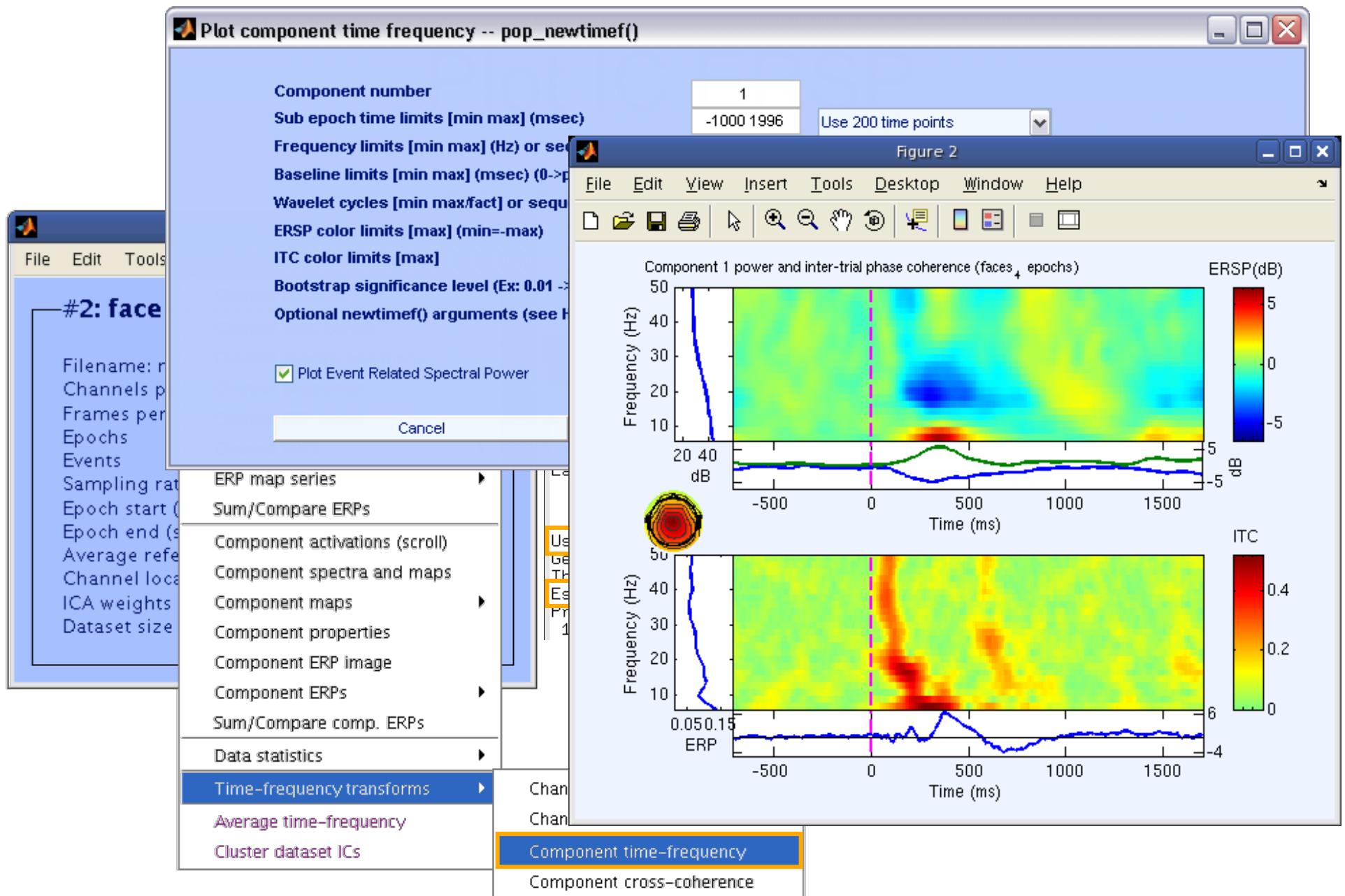


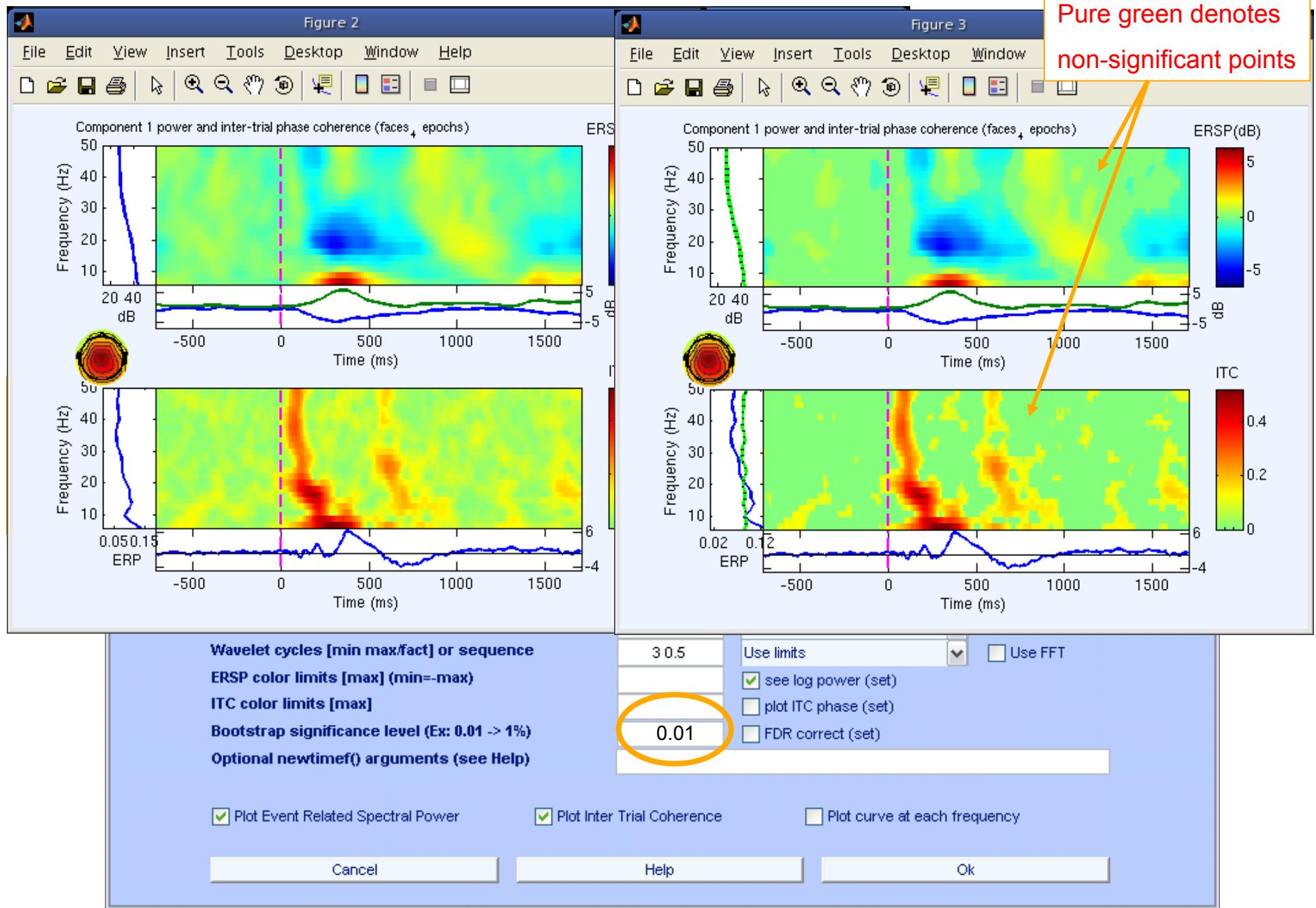
*Attend left-stim right*

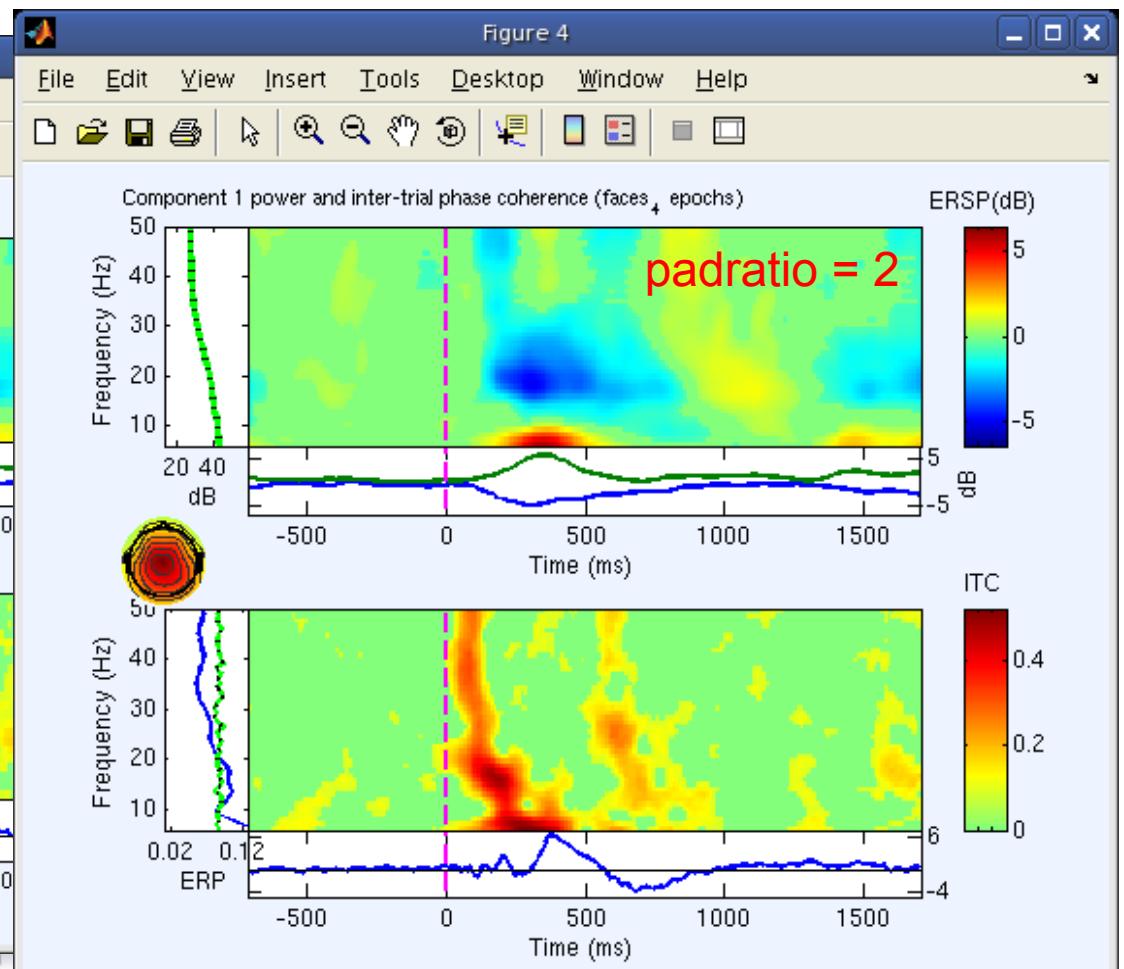
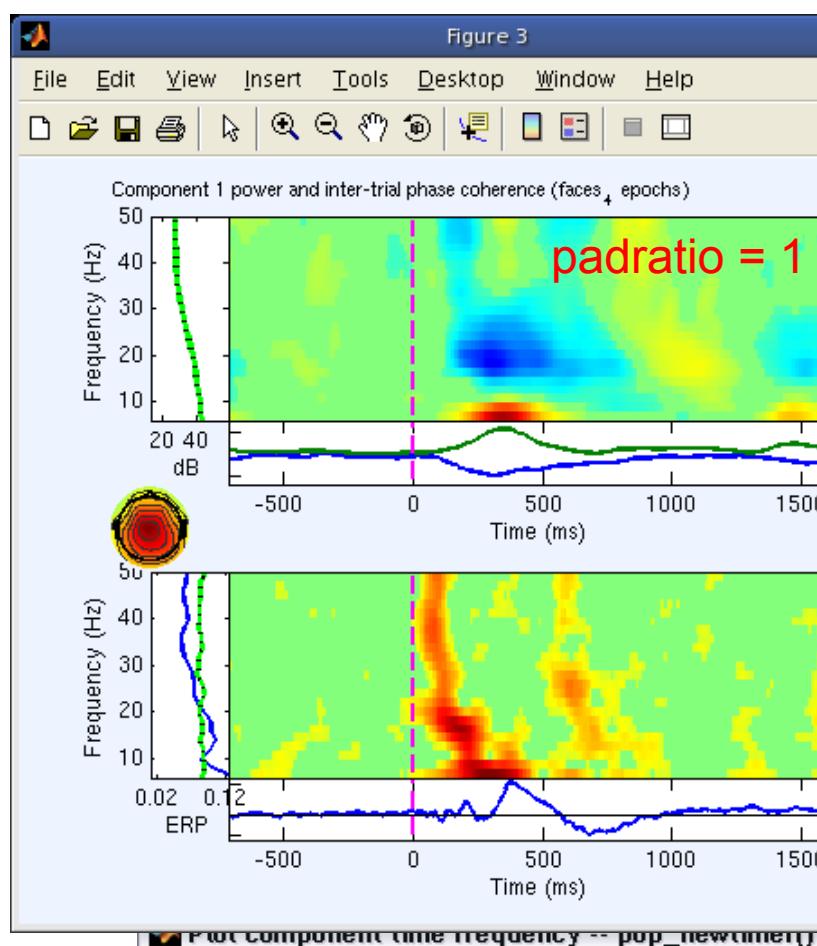


*Difference*









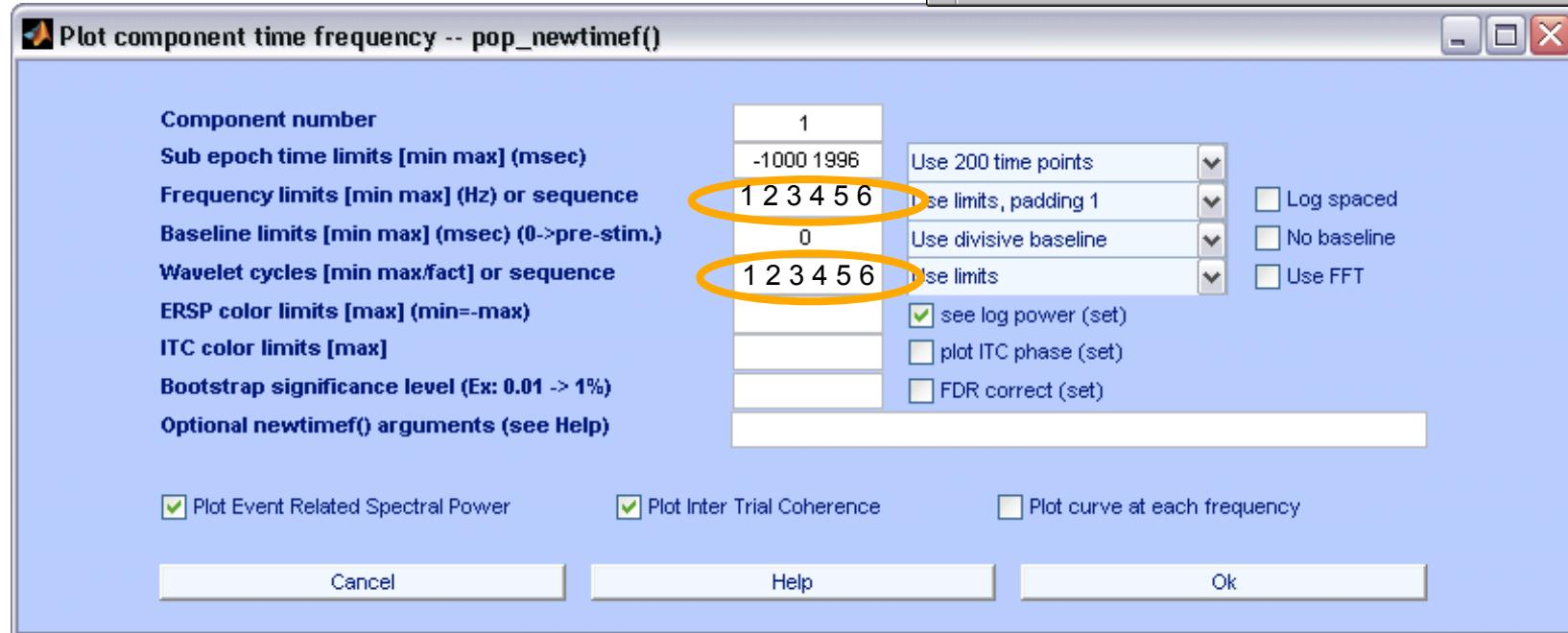
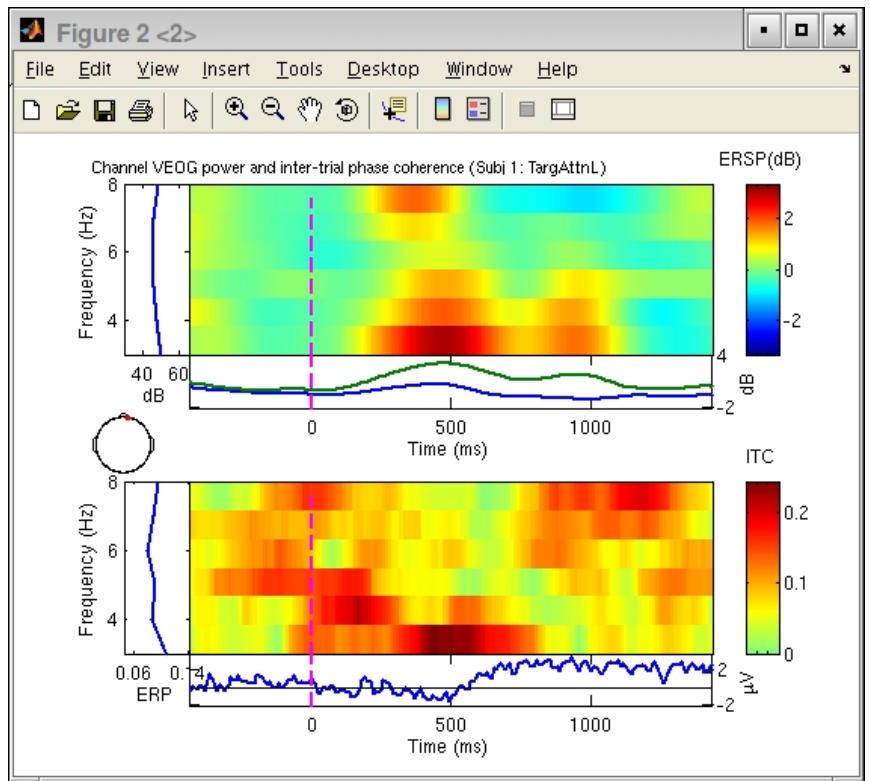
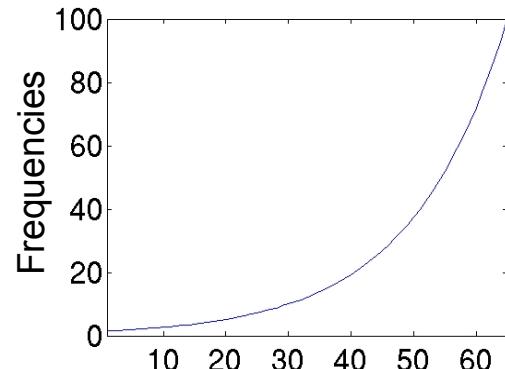
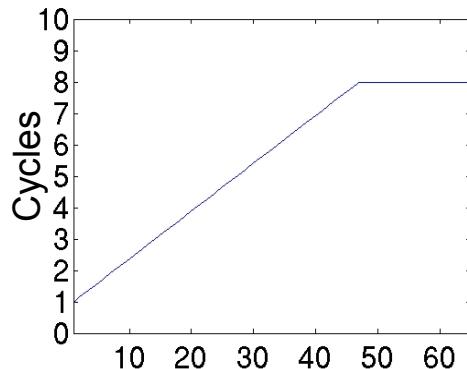
Increase  
# freq bins

Component number	1
Sub epoch time limits [min max] (msec)	-1000 1996
Frequency limits [min max] (Hz) or sequence	Use 200 time points
Baseline limits [min max] (msec) (0->pre-stim.)	Use limits, padding 1
Wavelet cycles [min max/fact] or sequence	Use divisive baseline
ERSP color limits [max] (min=-max)	Use limits
ITC color limits [max]	<input checked="" type="checkbox"/> see log power (set)
Bootstrap significance level (Ex: 0.01 > 1%)	<input type="checkbox"/> plot ITC phase (set)
Optional newtimef() arguments (see Help)	<input type="checkbox"/> FDR correct (set)

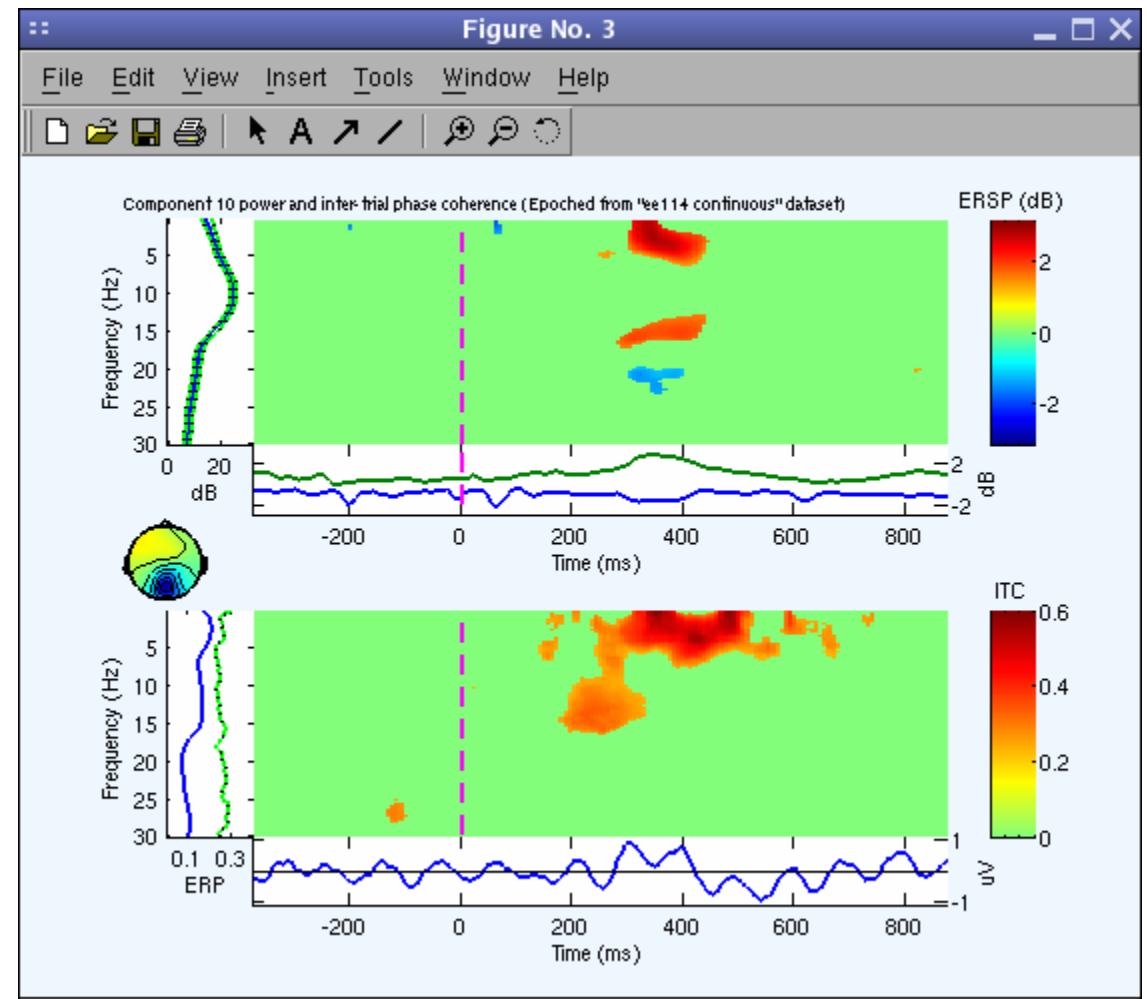
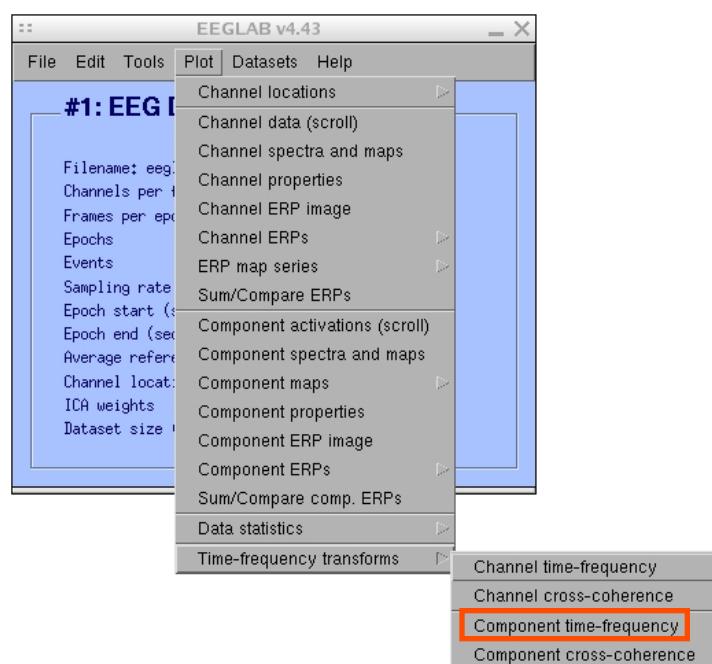
Plot Event Related Spectral Power     
  Plot Inter Trial Coherence     
  Plot curve at each frequency

## To visualize both low and high frequencies

```
freqs = exp(linspace(log(1.5), log(100), 65));
cycles = [ linspace(1, 8, 47) ones(1,18)*8 ];
```

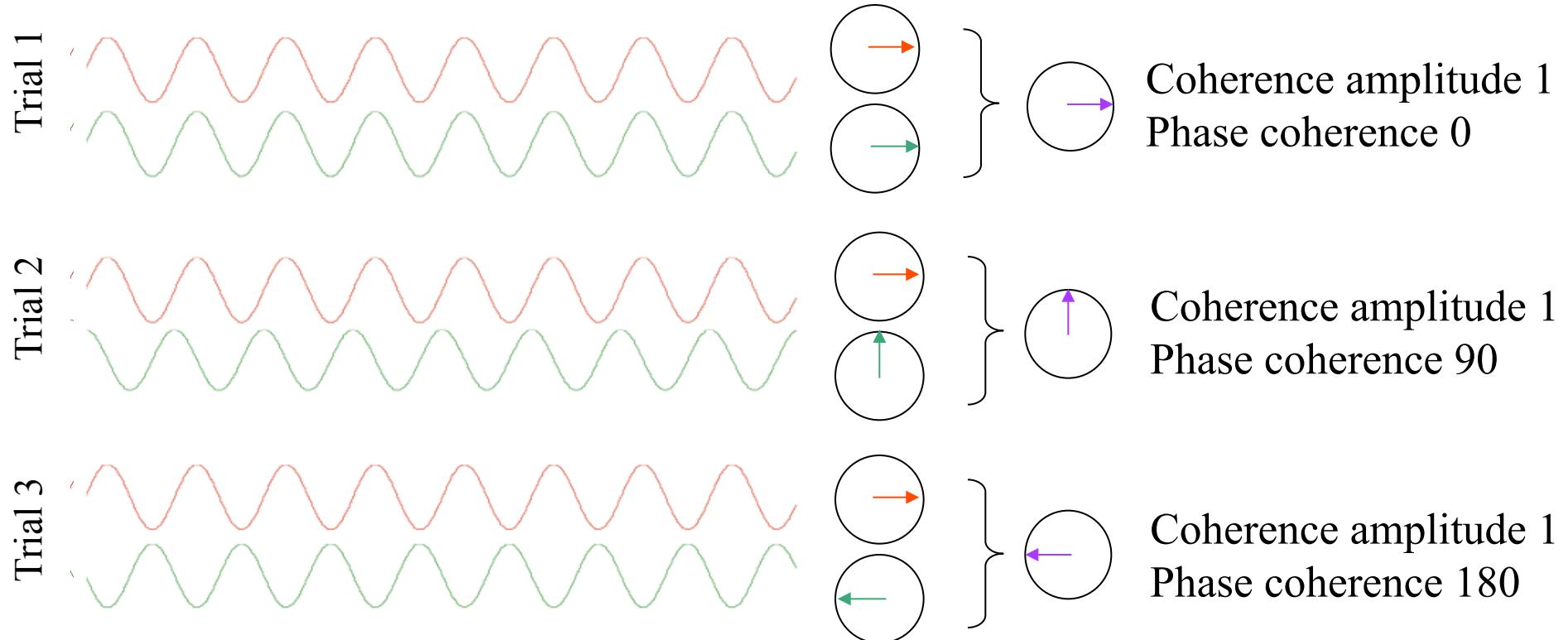


# Component time-frequency

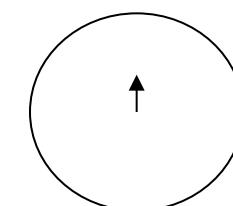


# Cross-coherence amplitude and phase

2 components, comparison on the same trials



$$\text{COHERENCE} = \text{mean}(\text{phase vector})$$



Norm 0.33  
Phase 90 degree

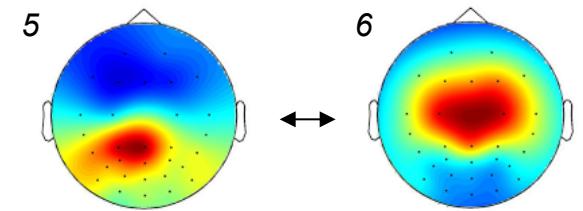
# Phase coherence (default)

$$ERPCOH^{a,b}(f,t) = \frac{1}{n} \sum_{k=1}^n \frac{F_k^a(f,t) F_k^b(f,t)^*}{|F_k^a(f,t)| |F_k^b(f,t)|}$$

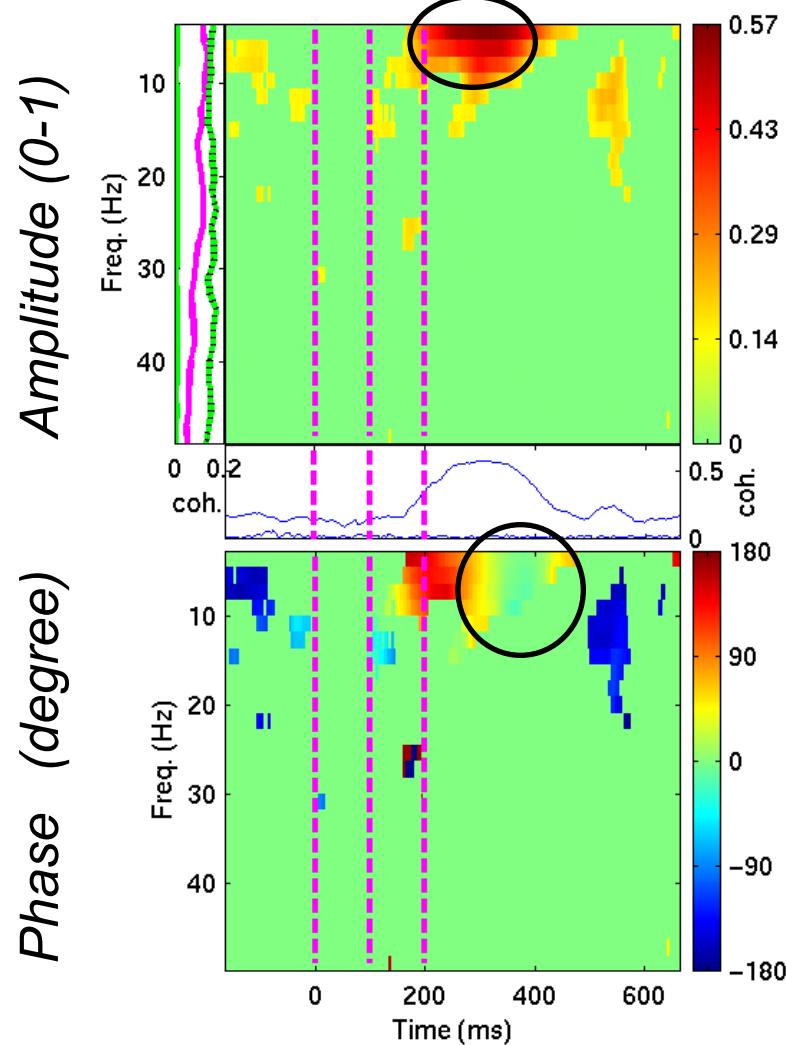
Only phase information component a

Only phase information component b

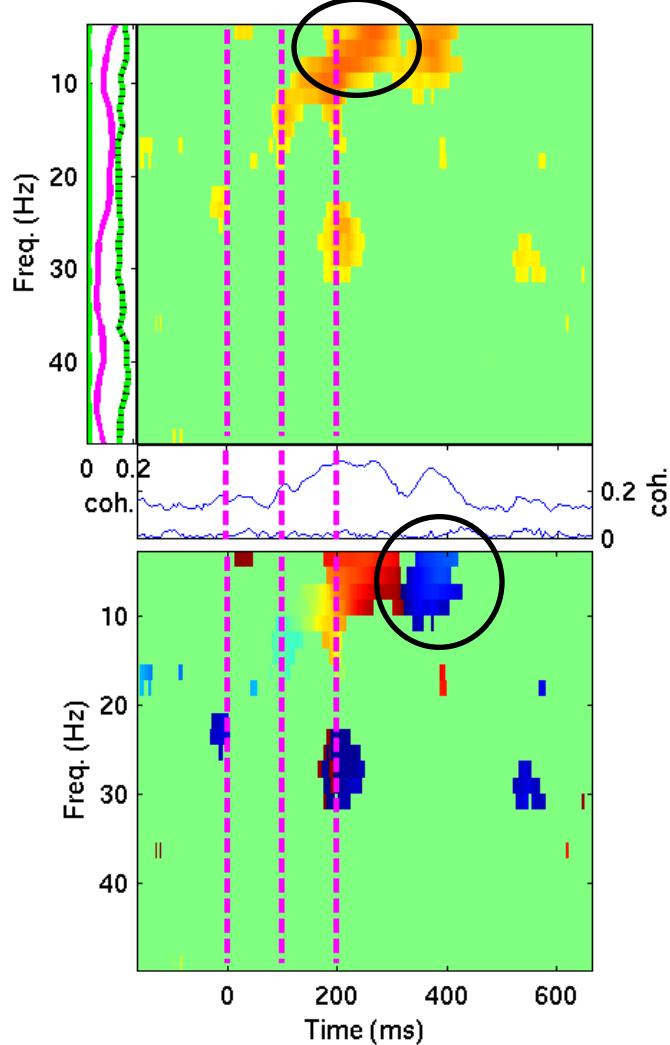
# Cross-coherence amplitude and phase

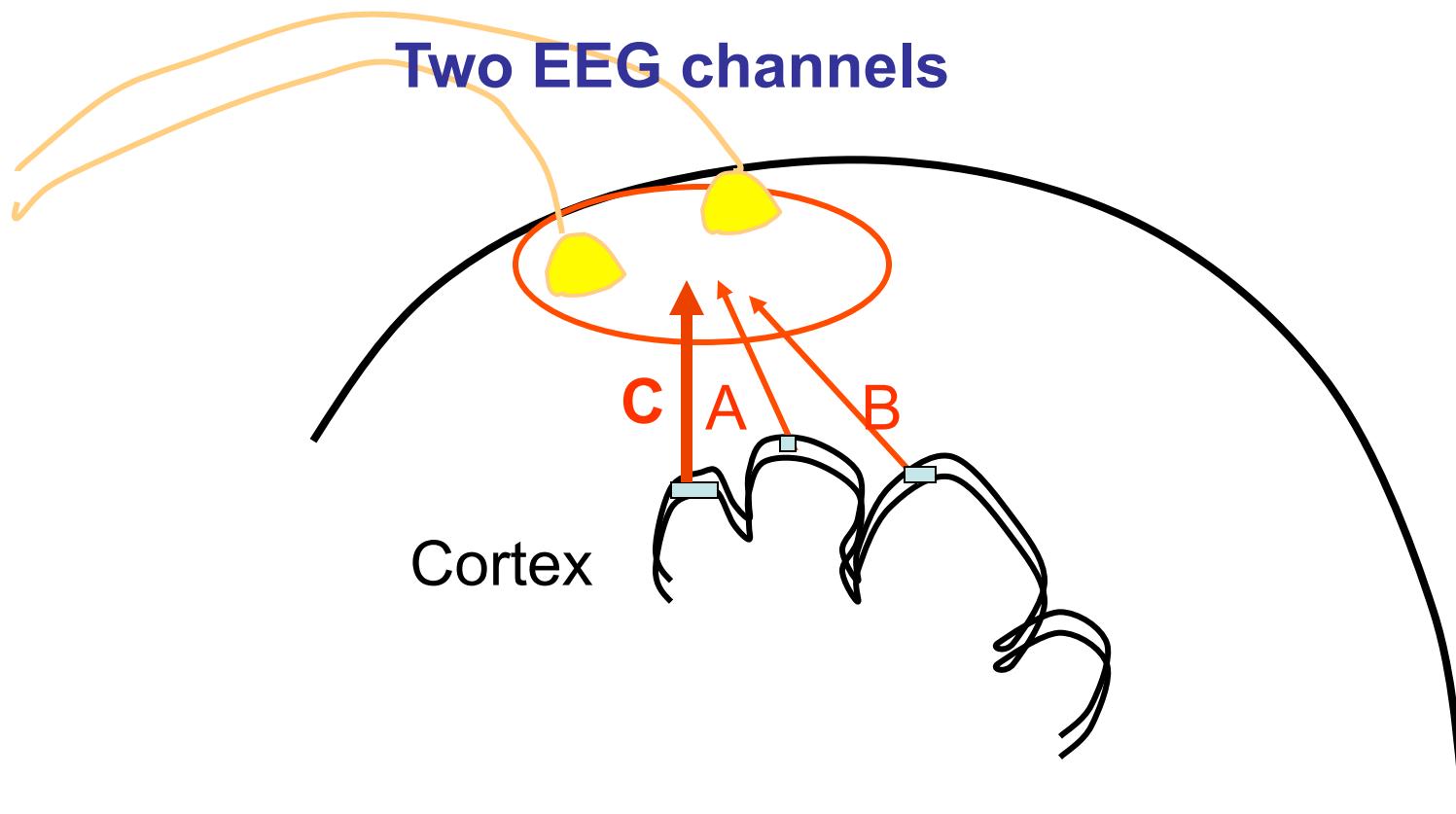


*Animal picture*

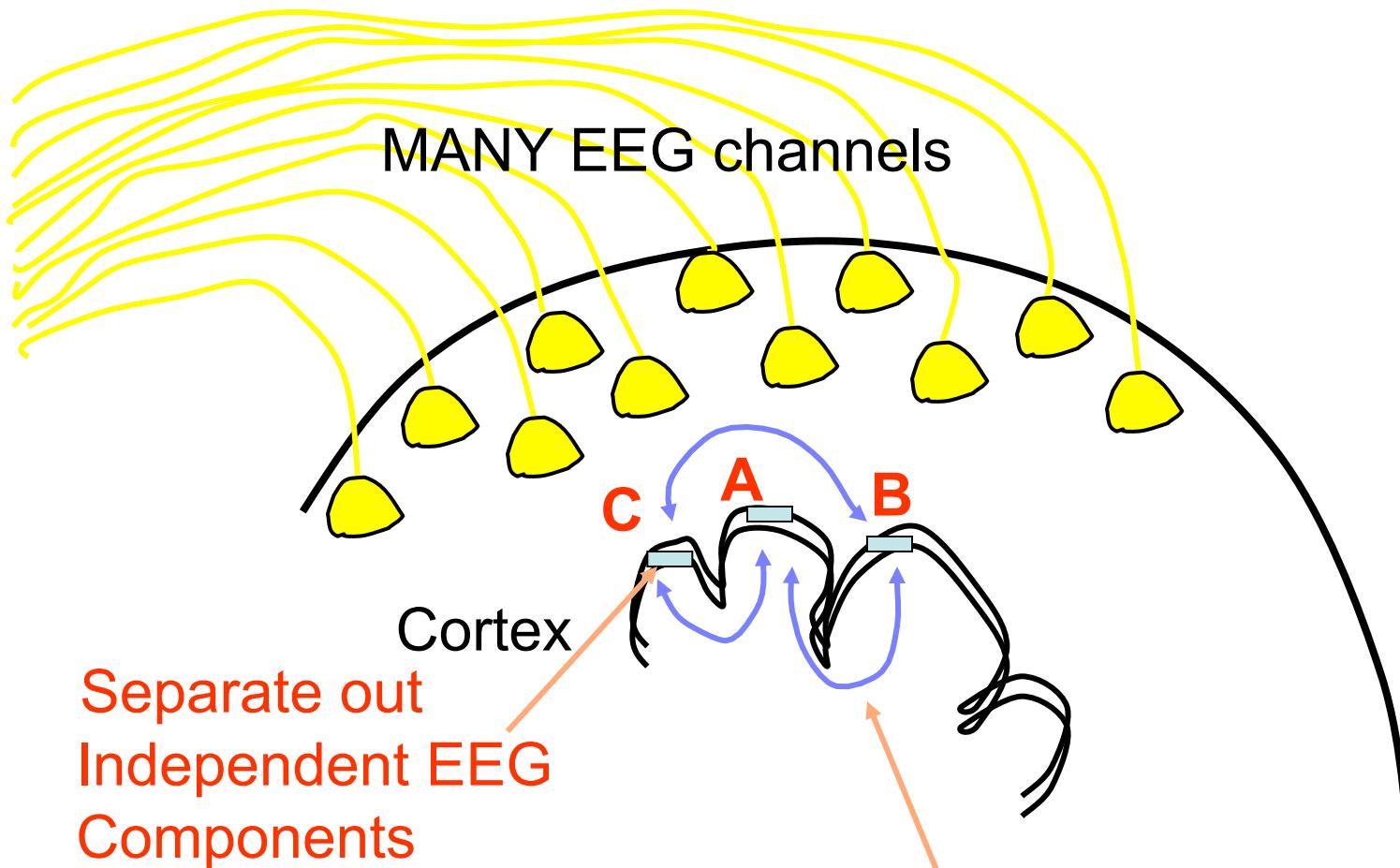


*Distractor picture*



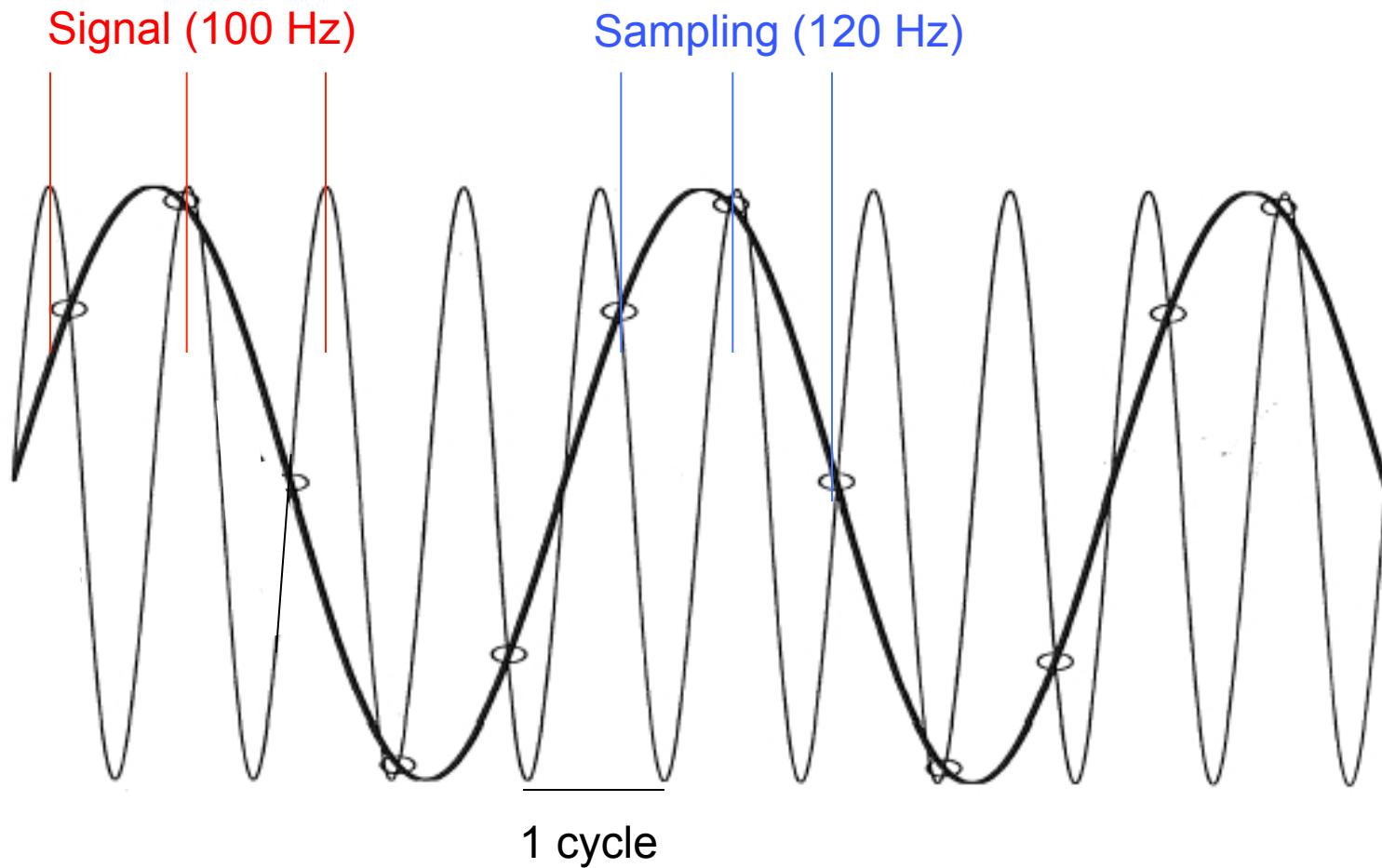


**Scalp channel coherence → source confounds!**



**source dynamics!**

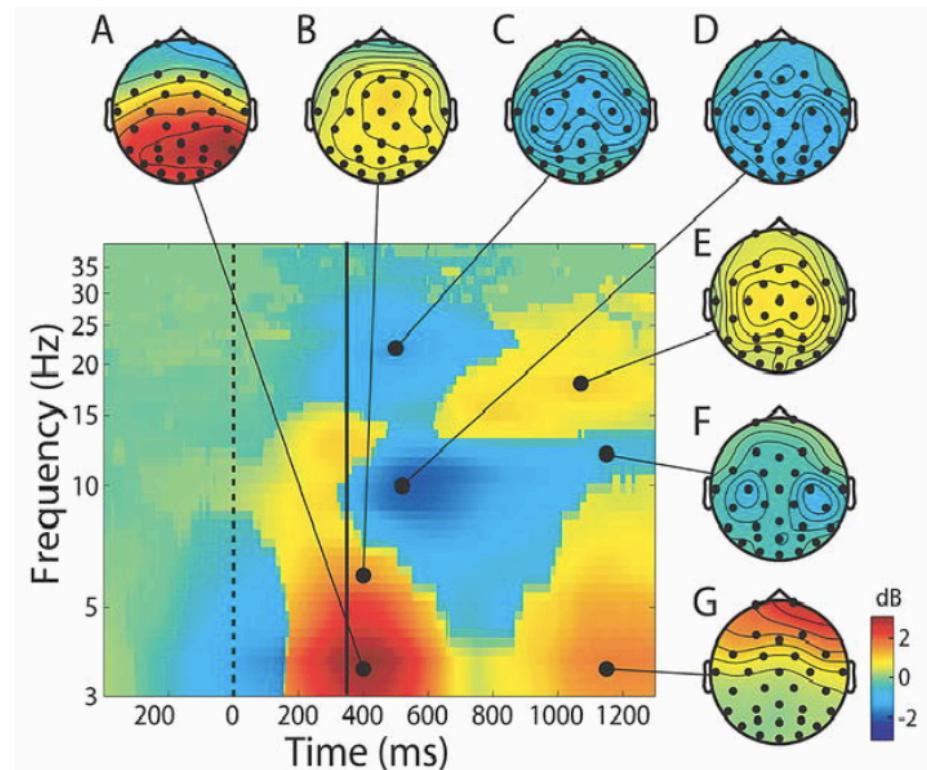
# Niquist frequency: Aliasing



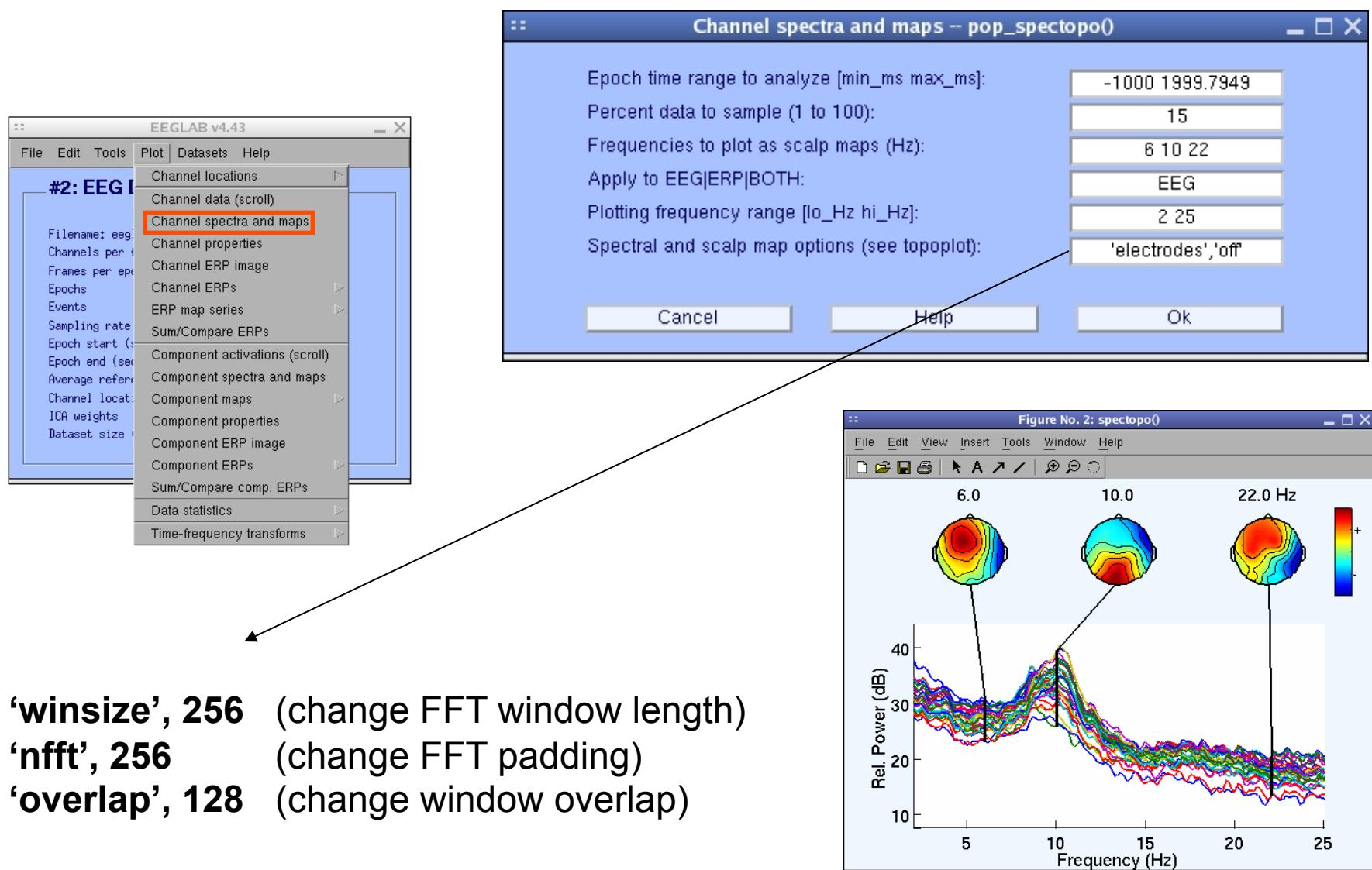
e.g. 100 Hz sampled at 120 Hz

# Advanced time-frequency functions

- Tftopo(): allow visualizing time-frequency power distribution over the scalp



# Plot data spectrum using EEGLAB



- **ALL**

Start EEGLAB, from the menu load  
`sample_data/eeglab_data_epochs_ica.set`  
or your own data (epoch, reject noise if not  
done already)

- **Novice**

From the GUI, Plot spectral decomposition  
with 100% data and 50% overlap ('overlap').  
Try reducing window length ('winsize') and  
FFT length ('nfft')

- **Intermediate**

Same as novice but using a command line  
call to the `pop_spectopo()` function. Use GUI  
then history to see a standard call ("eegh").

- **Advanced**

Same as novice but using a command line  
call to the `spectopo()` function.

## Exercise

