#### ComputerLab - Compressive sensing and application to MRI - Python Version

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This computer lab addresses the implementation and analysis of reconstruction algorithms for compressive sensing. In particular, an application to medical resonance imaging (MRI) is addressed. The goal is to show the connection between compressive sensing and denoising. To get an intuition, this lab first explores synthetic 1D sparse signals.

This computer lab employs Python. You can also use jupyter notebook.

## 1 Denoising sparse 1D signals

Create a script file called tp1.py (or tp1.ipynb) that contains all instructions described below.

1.1. Generate a  $1 \times n$  vector, x, with k non-zero ((1:k)/k) coefficients where n = 128, k = 5, and permute them randomly.

Create a graph reporting the signal as a function of the position in the vector. For each plot add labels, titles. You can use latex in the titles. (hint: test the pyplot function stem)

- 1.2. Add random Gaussian noise with standard deviation  $\sigma = 0.05$  to the signal, y = x + N. Create a graph showing the noisy signal.
- 1.3. One approach for denoising consists in using regularization with Tichonov penalty to estimate the signal from noisy data. More precisely, it solves for  $\lambda \geq 0$ :

$$\hat{x} = \arg\min_{z \in \mathbb{R}^n} \frac{1}{2} ||z - y||_2^2 + \lambda \frac{1}{2} ||z||_2^2 \tag{1}$$

This optimization trades the norm of the solution with data consistency. This approach has two advantages: (i) it has a closed form solution, (ii) the estimate is a linear function of the noisy data. Derive the closed-form solution for Tichonov regularization.

- 1.4. Create a graph showing the reconstructed signal for  $\lambda \in \{0.01, 0.05, 0.1, 0.2\}$ . Why is the solution  $\hat{x}$  not sparse?
- 1.5. Instead of Tichonov regularization, which penalizes the  $l_2$  norm, we will use the  $l_1$  norm penalized solution. More precisely, we will solve for  $\lambda \geq 0$ :

$$\hat{x} = \arg\min_{z \in \mathbb{R}^n} \left( \frac{1}{2} ||z - y||_2^2 + \lambda ||z||_1 \right)$$
 (2)

Show that the problem admits a closed form solution, and that this solution is

$$\hat{x} = \sigma_{\lambda}(y) = \begin{cases} y_l + \lambda & if \quad y_l \le -\lambda \\ 0 & if \quad |y_l| < \lambda \end{cases} \quad \forall l \in \{1, ..., n\}$$

$$y_l - \lambda & if \quad y_l \ge \lambda$$

$$(3)$$

In the course, the Basis Pursuit (BP) algorithm has been used instead of a closed form solution. What is the difference between (2) and the problem solved by BP? Do you know (2) under another name?

1.6. The function (3) is often referred to as soft-thresholding or shrinkage. Write a function called SoftThresh, that implements (3).

Plot SoftThresh $(u, \lambda)$  for  $u \in [-10, 10]$  and  $\lambda = 2$ . (Note that the function is implemented for a vector

of length n, here you have to plot the result for a vector of length 1). Describe what happens when  $y_l$  is small compared to  $\lambda$ , and when  $y_l$  is large.

1.7. Apply SoftThresh to the noisy signal y for  $\lambda \in \{0.01, 0.05, 0.1, 0.2\}$ . Is the solution  $\hat{x}$  sparse? Is the solution  $\hat{x}$  the same as x? In particular, compare the position and the value of the non-zero coefficients.

## 2 Random Frequency Domain Sampling and Aliasing

We'll now explore the connection between compressive sensing and denoising and the importance of choosing a good measurement matrix. To do so, we'll observe the effect of regular and then random sampling of the signal in the frequency domain.

Create a script file called tp2 that contains all instructions described below.

- 2.1. Same as Part 1. Generate a  $1 \times n$  vector, x, with k non-zero ((1:k)/k) coefficients where n = 128, k = 5, and permute them randomly.
- Create a graph reporting the signal as a function of the position in the vector.
- 2.2. Compute the Fourier transform of the sparse signal, X = Fx where F is a Fourier transform operator. Create a graph reporting the signal X as a function of the position in the vector.

In the following, we will measure a subset of the Fourier transform,  $X_u = F_u x$  where  $F_u$  is a Fourier transform evaluated only at a subset of frequency domain samples. This is an underdetermined data set for which there is an infinite number of possible solutions. However, we do know that the original signal is sparse, so there is hope we will be able to reconstruct it. This technique of subsampling the Fourier transform coefficients can be seen as a compressive sensing technique. Indeed, in compressive sensing, we take less measurements than dictated by the Shannon-Nyquist criterion and take linear combinations of the signal. More formally, we compute y = Mx, where M is a matrix with more columns than rows.  $F_u$  is an example of such a compressive sensing measurement matrix. The theory of compressive sensing suggests random undersampling. To see why, we will look at (non random) equispaced undersampling and compare it to random undersampling.

- 2.3. Undersample the Fourier transform coefficients by taking 32 equispaced samples. Compute the inverse Fourier transform, filling the missing data (in the frequency domain) with zeroes, and multiply it by 4 to correct for the fact that we have only 1/4 of the samples.
- Plot the real and imaginary parts of xu: real(xu) imag(xu). You should observe that xu is a periodic version of x. Why? Will we be able to reconstruct the original signal from the result?
- 2.4. Now, undersample X by taking 32 samples at random. Compute the zero-filled inverse Fourier transform and multiply by 4 again,

Plot the real and imaginary parts of xr: real(xr) imag(xr). (Use the Matlab functions stem, hold on/off). Describe the result. Will we be able to reconstruct the signal from the result? How does this resemble a denoising problem? And how does this differ from a denoising problem?

# 3 Reconstruction from Randomly Sampled Frequency Domain Data

Create a new script file called tp3 that contains all instructions described below.

3.1. Same as Part. Generate a  $1 \times n$  vector, x, with k non-zero ((1:k)/k) coefficients where n = 128, k = 5, and permute them randomly. Plot x.

Create a graph reporting the signal as a function of the position in the vector. Add the title "original signal x".

Same as Part 2: compute the Fourier transform X and undersample X by taking 32 samples at random. This leads to y, the acquired signal. Create a graph reporting the acquired signal as a function of the

position in the vector. Add the title "acquired signal y".

Note that here the acquired signal y is a n-length vector, containing "0" and the "true" acquired samples. This will ease the implementation.

3.2. Modify SoftThresh to handle complex signals

$$\hat{x} = \sigma_{\lambda}(y) = \begin{cases} 0 & if \quad |y_l| < \lambda \\ \frac{y_l}{|y_l|} (|y_l| - \lambda) & if \quad |y_l| \ge \lambda \end{cases} \quad \forall l \in \{1, ..., n\}$$

$$(4)$$

and test this function.

3.3. We will now estimate x by taking into account the fact that x is sparse.

To do so, we will implement the Projection Over Convex Sets (POCS) algorithm described below. This algorithm consists in iteratively applying soft-thresholding and constraining data consistency. First, we initially set  $\hat{X}_0 = y$ . Then, we implement the following iteration

- 3.3.1. Compute the inverse Fourier transform to get an estimate of the signal:
- $\hat{x}_i = F^{-1}\widehat{X}_i = F^*\widehat{X}_i$  (F is unitary).
- 3.3.2. Apply SoftThresh  $\hat{x}_i = \sigma_{\lambda}(\hat{x}_i)$  in the signal domain (where the signal is sparse)
- 3.3.3. Compute the Fourier transform  $\hat{X}_i = F\hat{x}_i$
- 3.3.4. Enforce data consistency in the frequency domain

$$\widehat{X}_{i+1}(j) = \begin{cases} \widehat{X}_i(j) & \text{if } y(j) = 0\\ y(j) & \text{otherwise} \end{cases}$$
 (5)

- 3.3.5. Stop after a fixed number of iteration. Another stopping criterion can be used: repeat until  $||\hat{x}_{i+1} \hat{x}_i|| < \epsilon$  (little changes of the estimate).
- 3.4. Apply the algorithm (at least 100 iterations) to the undersampled signal with  $\lambda \in \{0.01, 0.05, 0.1\}$  and plot the reconstructed signal at each iteration.
- 3.5. Make a plot of error between the true x and the estimate at each iteration  $x_i$  as a function of the iteration number i, plotting the result for each of the  $\lambda$ 's.Comment.
- 3.6. Now, repeat the iterative reconstruction for the equispaced undersampled signal. What's wrong?

### 4 Phase transition

In the same file tp3

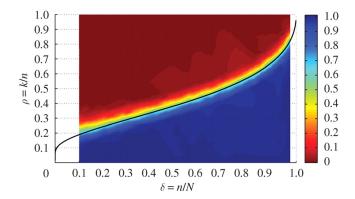
We've seen that with the combination of sparsity, incoherent measurements and a sparsity based reconstruction, compressed sensing can exactly reconstruct a 5-sparse signal with 4 times undersampling. But how well does compressed sensing work with other sparsity level and undersampling factor? For bandlimited signals, we have the Nyquist rate guiding our sampling strategy. For compressed sensing we will instead look at the phase transition diagram.

The phase transition diagram is a 2D color plot that can characterize signal recovery performance. On its horizontal axis we have the undersampling factor  $\delta = ($  Number of measurements n / Signal length N), and its vertical axis, we have the sparsity level  $\rho = ($  Number of nonzeros k / Number of measurements n). At each point on the 2D plot, we assign the probability of exactly recovering the signal as its value (with a probability of 1 being what we want), so the resulting plot is a color plot.

In general, there will be a transition between a success region on the bottom right to a failure region on the top left in the phase transition diagram. This is because given the same number of measurements, more nonzeros in your signal will also make the recovery harder. Similarly, given the same sparsity level, less measurements will make the recovery harder.

For compressed sensing, it turns out there is a very sharp transition between success and failure in the phase transition diagram. Below the phase transition curve, we recover the signal exactly with

probability almost 1. Above the phase transition curve, we can recover the signal exactly with probability almost 0. This transition curve essentially generalizes the Nyquist rate. Instead of depending on the signal bandwidth, our sampling rate now depends on the sparsity level.



The above figure shows a compressed sensing phase transition diagram from random Fourier measurements. This figure is taken from the paper Observed universality of phase transitions in high-dimensional geometry, with implications for modern data analysis and signal processing by Donoho and Tanner. For each point on the diagram, the authors generate 200 random instances of the compressed sensing problem and then calculate the frequency of success as the success rate. From the diagram, we can clearly see the phase transition curve, splitting the diagram into a success region and a failure region. The phase transition curve is theoretically justified, but the details are beyond the scope of the course.

In the following part, we will empirically generate a simple version of the phase transition diagram. Instead of generating 200 instances and assigning the probability of success, for each point in the diagram, we will assign the normalized mean square error between the recovered signal and the original signal for 8 compressed sensing problem instances. We will consider a length 128 signal and a 32x32 discretized phase transition diagram. For each  $\delta$  and  $\rho$ , we will do the following four steps:

- Randomly generate a sparse vector according to  $\rho$
- Take random measurements in the Fourier domain according to  $\delta$
- Reconstruct the signal using the iterative reconstruction algorithm Compute the normalized error with the original sparse vector.
- 4.1 For convenience, first create a function  $x_rec = cs_recon(Y, lamb, niter)$  that takes in the randomly subsampled Fourier measurements Y, the threshold lamb and the number of iterations niter and returns the iteratively reconstructed signal  $x_i$
- 4.2 Next, initialize the phase transition matrix as a 32x32 zero matrix. We will consider a scaled version of  $\delta$  and  $\rho$  by N=128 and loop through 32 steps from 0 to 127. For each  $\delta$  and  $\rho$ , you should generate a randomly signed k-sparse vector with  $k=\delta\rho/128$ .

```
k = np.floor(rho * delta / 128)
x_orig = np.append( np.sign(np.random.randn(k)) , np.zeros( (1,128-k) ) )
x_orig = x_orig[ np.random.permutation(128) - 1 ]
X_orig = np.fft.fft(x_orig)
```

Then generate a randomly undersampled spectrum Y with  $\delta$  number of measurements and reconstruct it just as we did in the first part of the exercise. Use  $\lambda = 0.05$  and 30 iterations. After reconstruction, add the normalized mean squared error to each point of the phase transition diagram:

```
phase_transition[rho / 4, delta / 4] +=
np.linalg.norm( x_rec - x_orig ) / (np.linalg.norm( x_orig ) + 1e-5)
```

Do the above steps 8 times and divide the resulting phase\_transition by 8. Your resulting code should have 3 for loops.

Generate the phase transition matrix and plot it using plt.imshow(). Note that it may take a while to generate the matrix. If you are impatient, you can put a print statement after the first for loop.

### 5 Reconstruction of MRI acquired through compressive sensing

Download the script file called tp4.ipynb that contains all instructions and questions we briefly described below.

We now evaluate the sparse approximation of an axial T2 weighted FSE image. Even without noise, medical images are generally not sparse. However, like natural images, medical images have a sparse representation in a transform domain, such as the wavelet domain. Here, we will use the PyWavelets package to perform wavelet transforms. The PyWavelet package does not provide nice functions for visualizing the wavelet transforms. To do this, we need to define functions that stack and unstack the approximation and detail coefficients, as well as scale the different levels when displaying an image. These functions are given in the file.

The temporal MRI signal (i.e. the raw data) directly samples the spatial frequency domain of the MR image. In other words, the measurements are the 2D-Fourier transform of the MR image i.e. a linear combination of the MR signal. These raw data are usually referred to as k-space.

Compressive sensing MRI consists in sampling the k-space at a rate lower than the Shannon-Nyquist criterion. In other words, it consists in subsampling in the spatial-frequency domain. This is similar to what we studied in Part 2 and 3. The difference is that we studied 1D pure sparse signal and now we will study 2D not perfectly sparse signals.

To reconstruct the MR image, we will perform the reconstruction of the wavelet transform of the MR image, and then compute the MR image.

Open the tp4 file, read the instructions, execute the cells contents and complete it if necessary.