

Graph-Theoretic Consistency for Robust and Topology-Aware Semi-Supervised Histopathology Segmentation (Student Abstract)

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Abstract

Semi-supervised semantic segmentation (SSSS) is vital in computational pathology, where dense annotations are costly and limited. Existing methods often rely on pixel-level consistency, which propagates noisy pseudo-labels and produces fragmented or topologically invalid masks. We propose **Topology Graph Consistency (TGC)**, a framework that integrates graph-theoretic constraints by aligning Laplacian spectra, component counts, and adjacency statistics between prediction graphs and references. This enforces global topology and improves segmentation accuracy. Experiments on GlaS and CRAG demonstrate that TGC achieves state-of-the-art performance under 5–10% supervision and significantly narrows the gap to full supervision.

Introduction

Semantic segmentation in histopathology is a key step for computational pathology, enabling analysis of tissue architecture and cancer grading. Yet, obtaining dense pixel-level annotations remains costly and requires expert effort, especially for complex glandular structures in colorectal tissues. Semi-supervised learning provides a practical solution by leveraging unlabeled data to improve segmentation with limited supervision (Le et al. 2025; Pham et al. 2025a). However, most existing methods enforce pixel-level consistency, which is prone to label noise and tends to produce fragmented or topologically invalid masks. These errors are particularly critical when gland morphology and lumen enclosure have diagnostic importance (Pham et al. 2025b).

Unlike pixels, region-level representations can model structural relationships between tissue components. Graph-based formulations are thus well suited for histopathology, as they naturally capture connectivity, adjacency, and topology between glandular regions (Felzenszwalb and Huttenlocher 2004; Kipf and Welling 2017; Zhang, Cui, and Zhu 2021). By reasoning over region graphs instead of individual pixels, segmentation models can preserve biologically meaningful topology and reduce the risk of inconsistent gland boundaries.

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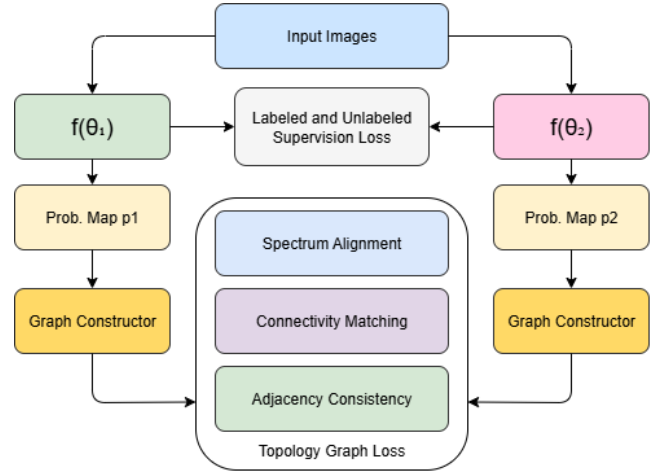


Figure 1: Overview of the proposed TGC framework. Two networks $f(\theta_1)$, $f(\theta_2)$ process labeled and unlabeled inputs, producing probability maps converted into graphs. Graph descriptors (spectrum, connectivity, adjacency) define the topology loss, complementing DiceCE supervision on labeled data and pseudo-label consistency on unlabeled data.

Motivated by this, we propose **Topology Graph Consistency (TGC)**, a dual-network semi-supervised framework that converts segmentation maps into region-level graphs and aligns them through spectral and structural constraints. TGC encourages both local accuracy and global topological coherence, resulting in more robust and morphologically faithful predictions. Experiments on the GlaS (Sirinukunwattana et al. 2017) and CRAG (Graham et al. 2019) datasets show that TGC achieves state-of-the-art results under 5–10% supervision, outperforming recent semi-supervised methods while better preserving gland topology.

Methodology

An overview of the proposed **Topology Graph Consistency (TGC)** framework is illustrated in Figure 1. We design a dual-network semi-supervised segmentation strategy with a novel topology-aware loss, which augments pixel-level su-

pervision with graph-theoretic constraints to enforce structural plausibility.

Labeled and Unlabeled Supervision. Two models $f(\theta_1), f(\theta_2)$ of the same architecture are trained jointly with Dice+CE loss. For an input x with reference label y (ground truth if labeled, or pseudo-label from the other model if unlabeled), the loss is:

$$\mathcal{L}_{DiceCE}(x, y) = \mathcal{L}_{DiceCE}(f(\theta_1; x), y) + \mathcal{L}_{DiceCE}(f(\theta_2; x), y). \quad (1)$$

This unified formulation covers both labeled (x_l, y_l) and unlabeled (x_u, \hat{y}) cases, where \hat{y} denotes the pseudo-label exchanged between models, reducing confirmation bias.

Graph Construction. Given a probability map $p \in [0, 1]^{H \times W}$, we extract centroids $\{c_i\}$ to represent gland regions and build a k -nearest neighbor graph. The adjacency, degree, and Laplacian are:

$$A_{ij} = \begin{cases} \exp\left(-\frac{\|c_i - c_j\|^2}{2\sigma^2}\right), & j \in kNN(i), \\ 0, & \text{otherwise,} \end{cases} \quad (2)$$

$$D = \text{diag}(A\mathbf{1}), \quad L = I - D^{-\frac{1}{2}}AD^{-\frac{1}{2}}.$$

Here c_i, c_j are centroid coordinates, σ controls affinity decay, k is the neighborhood size, A is the weighted adjacency, D the degree matrix, and L the normalized Laplacian.

Topology Graph Loss. Given prediction graph G_p and reference graph G_r , we define:

$$\mathcal{L}_{spec} = \frac{1}{m-1} \sum_{i=2}^m (\lambda_i^{(p)} - \lambda_i^{(r)})^2, \quad (3)$$

where λ_i are Laplacian eigenvalues.

$$\mathcal{L}_{conn} = (\hat{k}(G_p) - \hat{k}(G_r))^2, \quad \hat{k}(G) = \sum_{i=1}^m \sigma((\tau - \lambda_i)\alpha), \quad (4)$$

where τ is a threshold and α a sharpness factor.

$$\mathcal{L}_{adj} = \frac{1}{\min(N_p, N_r)} \|\text{sort}(D_p) - \text{sort}(D_r)\|_2^2 + (\bar{A}_p - \bar{A}_r)^2. \quad (5)$$

Here D_p, D_r are degree vectors and \bar{A} the mean adjacency.

The total topology loss is:

$$\mathcal{L}_{TGC} = w_{spec}\mathcal{L}_{spec} + w_{conn}\mathcal{L}_{conn} + w_{adj}\mathcal{L}_{adj}, \quad (6)$$

with $w_{spec}, w_{conn}, w_{adj}$ as balancing weights.

Total Objective. The complete objective integrates pixel and graph-level supervision:

$$\mathcal{L}_{total} = \mathcal{L}_{DiceCE}^{(l)} + \lambda_{sup}\mathcal{L}_{TGC}^{(l)} + \mathcal{L}_{DiceCE}^{(u)} + \lambda_{unsup}\mathcal{L}_{TGC}^{(u)}. \quad (7)$$

Here $\lambda_{sup}, \lambda_{unsup}$ control the strength of topology regularization, with λ_{unsup} ramped up during training to mitigate early pseudo-label noise.

Dataset	Ratio	Method	Dice	Jaccard
GlaS	5%	CCVC	80.8	68.9
		CorrMatch	79.9	67.8
		FDCL	81.6	70.2
		Ours	82.7	71.8
	10%	CCVC	83.8	73.5
		CorrMatch	83.3	72.6
		FDCL	84.4	74.5
		Ours	85.2	74.8
CRAG	5%	CCVC	73.3	60.5
		CorrMatch	69.1	55.4
		FDCL	74.6	61.9
		Ours	75.1	62.9
	10%	CCVC	75.0	62.3
		CorrMatch	74.9	61.9
		FDCL	76.3	63.9
		Ours	79.6	67.9

Table 1: Results on GlaS and CRAG (Dice/Jaccard, %). Values are the mean over 5-fold cross-validation. Best in **bold**, second-best underlined.

Experiments

Implementation. We implement all experiments in PyTorch on a single NVIDIA RTX 3060 GPU (16GB), using DeepLabV3+ with a ResNet-101 backbone. Models are trained for 80 epochs on GlaS and 120 epochs on CRAG, with all images resized to 256×256 . Standard data augmentations (random flips and rotations) are applied. We use AdamW optimizer (learning rate 1×10^{-4} , weight decay 0.05), batch size 8, and select the best validation checkpoint for inference. Our Topology Graph Consistency (TGC) loss is integrated into the dual-network training objective. All results are averaged over 5-fold cross-validation.

Results. As shown in Table 1, the proposed TGC framework consistently achieves top performance under both 5% and 10% supervision, outperforming or matching recent methods such as CCVC (Wang et al. 2023), CorrMatch (Sun et al. 2024), and FDCL (Nguyen et al. 2025). In addition to quantitative improvements, qualitative results show that TGC yields fewer fragmented predictions and better preserves glandular structures.

Conclusion and Future Work

We proposed **Topology Graph Consistency (TGC)**, a semi-supervised segmentation framework that enforces topological alignment via graph-based constraints. By leveraging spectral, connectivity, and adjacency cues, TGC improves structural consistency and segmentation under limited supervision, highlighting the value of topology-aware learning in medical imaging. In future work, we plan to extend TGC to diverse modalities and structures, and explore more expressive graph forms like hypergraphs to capture higher-order region relations. We will also investigate advanced reasoning modules, such as topology-aware GNNs or attention mechanisms, to further enhance segmentation robustness.

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