Histograms should not be used to segment functional lung MRI

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Abstract

Magnetic resonance imaging using hyperpolarized gases has facilitated the novel visualization of airspaces, such as the human lung. The advent and refinement of these imaging techniques have furthered research avenues with respect to the growth, development, and pathologies of the pulmonary system. In conjunction with the improvements associated with image acquisition, multiple image analysis strategies have been proposed and developed for the quantification of hyperpolarized gas images with much research effort devoted to semantic segmentation, or voxelwise classification, into clinically-oriented categories based on functional ventilation levels. Given the functional nature of these images and the consequent complexity of the segmentation task, many of these algorithmic approaches reduce the complex spatial image intensity information to intensity-only considerations, specifically those associated with the intensity histogram. Although significantly simplifying computational processing, this transformation results in the loss of important spatial cues for identifying salient imaging features, such as ventilation defects, which have been identified as correlating with lung pathophysiology. In this work, we demonstrate the interrelatedness of the most common approaches for histogram-based, ventilation segmentation of hyperpolarized gas lung imaging for driving voxelwise classification. We evaluate the underlying assumptions associated with each approach and show how these assumptions lead to suboptimal performance. We then illustrate how a convolutional neural network can be constructed in a multi-scale, hierarchically feature-based (i.e., spatial) manner which circumvents the problematic issues associated with existing intensity-only approaches. Importantly, we provide the entire evaluation framework, including this newly reported deep learning functionality, as open-source through the well-known Advanced Normalization Tools (ANTs) library.

Introduction

Early acquisition and development

Early hyperpolarized gas pulmonary imaging research reported findings in qualitative terms.

Descriptions:

- "^{3}He MRI depicts anatomical structures reliably" (1)
- "hypointense areas" (2)
- "signal intensity inhomogeneities" (2)
- "wedge-shaped areas with less signal intensity" (2)
- "patchy or wedge-shaped defects" (3)
- "ventilation defects" (4)
- "defects were pleural-based, frequently wedge-shaped, and varied in size from tiny to segmental" (4)

Historical overview of quantification

Initial attempts at quantification of ventilation images were limited to ennumerating the number of "ventilation defects" or estimating ventilation defect percentage (as a percentage of total lung volume). Often these measurements were acquired on a slice-by-slice basis.

Prior to the popularization of deep learning in medical image analysis, including in the field of hyperpolarized gas imaging (5), widely used semi-automated or automated segmentation techniques were primarily based on intensity-only considerations. In order of increasing sophistication, these techniques can be categorized as follows:

- binary thresholding based on relative intensities (6),

- linear intensity standardization based on global rescaling of the intensity histogram to a reference distribution based on healthy controls, i.e., "linear binning" (7),
- non-linear intensity standardization based on piecewise linear transformation of the intensity histogram using the K-means algorithm (8), and
- Gaussian mixture modeling (GMM) with spatial constraints using Markov random field (MRF) modeling (9).

The early semi-automated technique used to compare smokers and never-smokers in (6) uses manually drawn regions to determine the mean signal intensity as well as the standard deviation of the noise to derive a threshold value of three noise standard deviations below the mean intensity. All voxels above that threshold value were considered "ventilated" for the purposes of the study. Similar to the histogram-only algorithms (i.e., linear binning and k-means), this approach does not take into account the various artefacts associated with MRI such as the non-Gaussianity of the imaging noise [@] and the intensity inhomogeneity field [@].

It is vitally important that it is understood that we are not claiming that these algorithms are erroneous. Much of the relevant research has been limited to quantifying differences with respect to ventilation vs. non-ventilation in various clinical categories and these algorithms have certainly demonstrated the capacity for advancing such research. However, as acquistion and analyses methodologies improve, so should the level of sophistication and performance of our measurement tools.

Methods

Results

Discussion

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