



Communication

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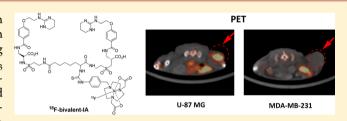
One-Step ¹⁸F Labeling of Non-Peptidic Bivalent Integrin $\alpha_{V}\beta_{3}$ **Antagonist for Cancer Imaging**

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Supporting Information

ABSTRACT: A rapid one-step ¹⁸F labeling reaction with fluoridealuminum complex, which is based on chelation chemistry, has received a surge of interest for ¹⁸F radiolabeling of peptides. In this study, a non-peptidic bivalent integrin $\alpha_y \beta_3$ antagonist (bivalent-IA) was conjugated with 1,4,7-triazacyclononane-1,4-diiacetic acid (NODA). A novel ¹⁸F labeled radiotracer, ¹⁸F-bivalent-IA, was developed via one step ¹⁸F-AlF/NODA chelation reaction in aqueous phase with high



radiochemical yield (65-75%, decay corrected) and good specific activity (750-850 mCi/µmol). The tumor integrin targeting efficiency and in vivo pharmacokinetic profile of ¹⁸F-bivalent-IA were evaluated in U-87 MG (integrin positive) and MDA-MB-231 (integrin negative) models by small-animal PET/CT scan followed by a biodistribution study. The PET/CT and ROI results showed high tumor uptake of ¹⁸F-bivalent-IA in U-87 MG tumor-bearing mice from 5 to 120 min p.i. with good contrast, and the U-87 MG tumor uptake values (6.35 \pm 0.67%ID/g, at 1 h p.i.) were 6 times higher than those of MDA-MB-231 tumor (1.05 \pm 0.12%ID/g, at 1 h p.i.) (P < 0.0001) which correlated with the integrin $\alpha_y \beta_3$ expression in tumor tissues confirmed by immunohistochemistry. Co-injection of the ¹⁸F-bivalent-IA with 6 nmol (6 µg) of nonradioactive bivalent-IA effectively blocked tumor uptake demonstrating the integrin $\alpha_y \beta_3$ -specificity. In conclusion, the first ¹⁸F labeled non-peptidic bivalent integrin $\alpha_y \beta_3$ targeting radiotracer, ¹⁸F-bivalent-IA, was developed and proved to be a highly potent and specific PET radiopharmaceutical for noninvasive imaging of integrin $\alpha_y \beta_y$, which plays a critical role in tumor angiogenesis and metastasis.

ositron emission tomography (PET) is a clinically used molecular imaging modality to detect cancer and other diseases with high sensitivity. Compared with other positron-emitting isotopes (11°C, 13°N, 15°O, 68°Ga, 89°Zr, 124°I), 18°F is the most widely used PET radioisotope because of suitable decay, low β^+ -trajectory, and small atomic size.^{2,3} Recently, the onestep ¹⁸F labeling method with fluoridealuminum complex, which is based on chelation chemistry, has received a surge of interest for peptide radiolabeling.^{4–8} In comparison with the classical ¹⁸F nucleophilic substitution reaction, which usually involves prosthetic groups with time-consuming multistep radiosynthesis, this new fluorination method is efficient, simple, and straightforward. As a novel chelator with $(Al^{18}F)^{2+}$ complex, 1,4,7-triazacyclononane-1,4-diiacetic acid (NODA) has excellent binding kinetics, and its Al¹⁸F complexes are highly stable in vivo. ^{9–13}

Integrin $\alpha_y \beta_3$, a receptor for extracellular proteins including vitronectin, fibronectin, and fibrinogen, plays an important role in tumor growth, angiogenesis, local invasiveness, and metastatic potential. 14–16 RGD peptides specifically binding to integrin $\alpha_{\nu}\beta_{3\nu}$ and their multivalent derivatives have been intensively studied with various radiolabels for noninvasively PET imaging of different cancer types. 6-8,17-20 In comparison with peptide/antibody, small molecules have advantages in developing the imaging moiety owing to their high affinity to target, low immunogenicity, and flexibility in chemical modification. At present, an ¹⁸F labeled small-molecule-based

integrin targeting radiotracer has not been reported. Our interest is to develop potent non-peptidic small molecular integrin $\alpha_v \beta_3$ targeting derivatives as a novel cancer theranostic platform. ^{21–24} We developed a bivalent-IA compound derived from a small molecule $\alpha_v \beta_3$ antagonist, 4-[2-(3,4,5,6-tetrahydropyrimidine-2-lamino)-ethyloxy]benzoyl-2-(S)-aminoethylsulfonyl-amino-h-alanine (Figure 1, IA) which exhibited subnanomolar range integrin receptor binding affinity (IC₅₀ = 0.40 ± 0.11 nM) and potent therapeutic efficacy as a single drug in a tumor xenographic model.^{23,24} In this study, we applied this facile and rapid ¹⁸F-AlF/NODA chelation method to synthetic small molecule radiolabeling and successfully developed, to the best of our knowledge, the first ¹⁸F labeled non-peptidic small molecule integrin $\alpha_{v}\beta_{3}$ targeted radiotracer, ¹⁸F-bivalent-IA. Small-animal PET revealed rapid, specific, and prominent uptake of ¹⁸F-bivalent-IA in human glioblastoma U-87 MG tumors (high integrin expression) but significantly lower and sporadic uptake in human breast cancer MDA-MB-231 tumors (low integrin expression) which successfully demonstrated the ability of ¹⁸F-bivalent-IA to quantitatively visualize integrin $\alpha_{\nu}\beta_{3}$ expression in vivo. The integrin $\alpha_{\nu}\beta_{3}$ expression in different tumor types was confirmed by

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Figure 1. Chemical structures of IA and ¹⁸F-bivalent-IA.

immunohistochemical (IHC) staining (see SI, Figure 1S) and was also indicated in the literature. With the significant tumor localization, excellent biodistribution, and pharmacokinetic properties, the radiotracer ¹⁸F-bivalent-IA used for tumor anti-angiogenic imaging and integrin-targeted therapy evaluation has great potential for future clinical translation.

The precursor bivalent-IA was obtained by a multistep synthesis according to our previously reported procedures. NODA-bivalent-IA was prepared by direct conjugation of bivalent-IA with NCS-MP-NODA (CheMatech, Dijon, France) in 75% yield. The compounds were purified by HPLC and were characterized by MS and NMR (see SI for details). To determine the receptor-binding ability, NODA-bivalent-IA was tested for its ability to competitively inhibit the attachment of

the natural ligand vitronectin to purified human $\alpha_v \beta_3$ (Chemicon International, CA) by enzyme-linked immunosorbent assay (ELISA) (see SI for details). The IC₅₀ value of NODA-bivalent-IA was 1.9 \pm 0.27 nM (see SI, Figure 3S) which demonstrated that NODA conjugation did not decrease the integrin $\alpha_v \beta_3$ receptor binding affinity.

In the radiolabeling reaction, NODA-bivalent-IA was radiolabeled by incubating with Na18F in 0.5 N NaOAc buffer (pH 4.0) at 100 °C for 15 min (see SI). The labeled product ¹⁸Fbivalent-IA (Figure 1, ¹⁸F-bivalent-IA) was then directly purified by C18 Classic Cartridge (Waters, Milford, MA). The whole radiosynthesis was accomplished within 25 min with a decay-corrected yield of 65-75% and radiochemical purity of more than 95% (n = 12). The specific activity of purified ¹⁸Fbivalent-IA was calculated as 750-850 mCi/µmol (27.8-31.6 MBq/µmol). Chemical stability of ¹⁸F-bivalent-IA was evaluated by radio-HPLC analysis that revealed no change in the chromatogram after 3 h incubation in mouse serum at 37 °C (see SI, Figure 2S). The radiolabeling and purification procedure of 18F-bivalent-IA, which was a one step reaction with no HPLC purification and no evaporation step, is less laborious and fully scalable for future commercial production.

Glioblastoma is one of the most aggressive tumors, and integrin α , β_3 is highly overexpressed in U-87 MG glioblastoma cells. $^{6,7,17-20}$ U-87 MG tumor was used to evaluate the in vivo pharmacokinetic profile and tumor targeting property of 18 F-bivalent-IA. 60 min dynamic small-animal PET/CT scans followed by static scans at 2 h after tail vein injection of 18 F-bivalent-IA were obtained using U-87 MG tumor-bearing mice (n=5 per group). Representative decay-corrected coronal images and regions of interest (ROI) analysis are shown in

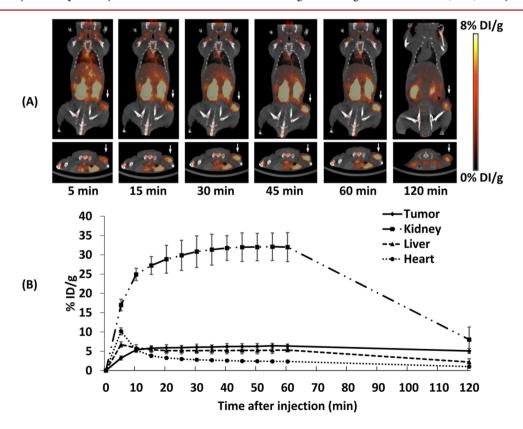


Figure 2. (A) PET/CT images of U-87 MG tumor-bearing mice injected intravenously with approximately 100 μ Ci of ¹⁸F-bivalent-IA. (B) Time—activity curves of tumor and major organs of U-87 MG tumor-bearing mice from 60 min dynamic scans after intravenous injection of ¹⁸F-bivalent-IA (n = 5). (Tumors are indicated by arrowheads.)

Figure 2. The U-87 MG tumors were clearly visualized with excellent tumor to background contrast for ¹⁸F-bivalent-IA as early as 5 min post injection. Compared with normal tissue, quantification of tumor-to-muscle ratios show that, for the U-87 MG tumor, tumor uptake values were over 30 times higher than those of the muscle at 1 h p.i (Figure 3E). From the ROI

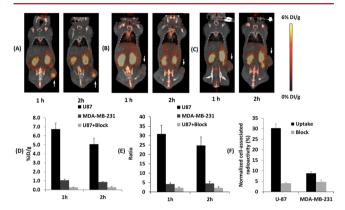


Figure 3. (A) PET/CT images of U-87 MG tumor-bearing mice injected intravenously with 18F-bivalent-IA, and (B) PET/CT images of U-87 MG tumor-bearing mice injected intravenously with ¹⁸F-bivalent-IA and 6 nmol (6 μ g) of bivalent-IA. (C) PET/CT images of MDA-MB-231 breast tumor-bearing mice injected intravenously with ¹⁸Fbivalent-IA. (Tumors are indicated by arrowheads.) (D) Quantitative analysis of small-animal PET/CT images. Comparison of decaycorrected ROI analysis of ¹⁸F-bivalent-IA (U-87 MG tumor-bearing mice) (n = 5), ¹⁸F-bivalent-IA (MDA-MB-231 breast tumor-bearing mice) (n = 3), and ¹⁸F-bivalent-IA coinjected with 6 nmol (6 μ g) of bivalent-IA (U-87 MG tumor-bearing mice) (n = 4) in tumor. (E) Comparison of tumor-to-muscle uptake ratios after injection of ¹⁸Fbivalent-IA (U-87 MG tumor-bearing mice) (n = 5), ¹⁸F-bivalent-IA (MDA-MB-231 breast tumor-bearing mice) (n = 3), and ¹⁸F-bivalent-IA coinjected with 6 nmol (6 μg) of bivalent-IA (U-87 MG tumorbearing mice) (n = 4). (F) Cell uptake and competition assay. Binding of ¹⁸F-bivalent-IA to U-87 MG and MDA-MB-231 cells with varying levels of integrin $\alpha_{v}\beta_{3}$.

analysis displayed in Figure 2B, in the first 15 min after tail vein injection, radioactivity rapidly accumulated in the tumor (5.80 \pm 0.65%ID/g) and was maintained throughout the entire scan process (5.07 \pm 0.66%ID/g, at 2 h p.i.). The tumor uptake peaked (6.42 \pm 6.3%ID/g) at 55 min p.i. In contrast, heart uptake peaked (10.18 \pm 0.9%ID/g) at 5 min p.i. but decreased to 2.68 \pm 0.29%ID/g at 20 min p.i. High radioactivity accumulated in the kidneys at 60 min p.i. (32.00 \pm 3.77%ID/g) and rapidly decreased at 2 h post injection (8.02 \pm 3.26%ID/g, at 2 h p.i.) demonstrating fast renal excretion. Low levels of liver uptake were also observed at all time points. The bone uptake was measured as 0.34 \pm 0.05%ID/g at 1 h p.i. and 0.20 \pm 0.07%ID/g at 2 h p.i., respectively, indicating good in vivo stability of the 18 F-bivalent-IA.

To further demonstrate $^{18}\text{F-bivalent-IA}$ for in vivo integrin $\alpha_v\beta_3$ receptor expression imaging, we also evaluated it using human breast MDA-MB-231 tumors with low integrin expression as a negative comparison. The PET/CT images of MDA-MB-231 breast tumor bearing mice of 1 h and 2 h postinjection are shown in Figure 3C. The MDA-MB-231 tumor uptake values were 1.05 \pm 0.12 and 0.86 \pm 0.06%ID/g at 1 and 2 h p.i. respectively, which were six times lower than those of the U-87 MG tumor (6.35 \pm 0.67%ID/g, at 1 h p.i. and 5.07 \pm 0.66%ID/g, at 2 h p.i., Figure 3D) (P < 0.0001). High integrin $\alpha_v\beta_3$ expression in U-87 MG tumors and low

expression in MDA-MB-231 tumors were confirmed by immunohistochemical (IHC) staining (see SI, Figure 1S). The in vitro cell uptake and blocking study of $^{18}\text{F-bivalent-IA}$ was also performed using U-87 MG and MDA-MB-231 cell lines (Figure 3F; for detailed procedures see SI). The radiotracer uptake levels revealed that $^{18}\text{F-bivalent-IA}$ represented a 4-fold-higher avidity with U-87 MG cells over MDA-MB-231 cells in vitro (P < 0.0001). The cell uptake was successfully blocked by coincubation with unlabeled bivalent-IA in U-87 MG cells which demonstrated specific binding to cell integrin $\alpha.\beta_3$ receptor.

The integrin $\alpha_{\nu}\beta_{3}$ specificity of ¹⁸F-bivalent-IA was confirmed by the blocking experiments in vivo. The PET/CT images at 1 and 2 h p.i. of U-87 MG tumor-bearing nude mice coinjected with ¹⁸F-bivalent-IA and 6 nmol (6 μ g) unlabeled bivalent-IA are shown in Figure 3B. The U-87 MG tumor uptake was effectively blocked to the background level. The ROI analysis (Figure 3D) showed that the uptake values were very low as 0.27 \pm 0.03 and 0.28 \pm 0.07%ID/g at 1 and 2 h p.i., respectively, in the blocking study.

Biodistribution studies were performed at 3 h postinjection after the microPET/CT scans for all imaging studies. Tumors and major organs were harvested, weighed, and the radioactivity was counted (Figure 4). The results demonstrated

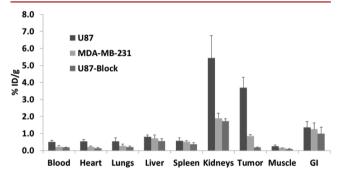


Figure 4. Biodistribution at 3 h postinjection ¹⁸F-NODA-bivalent-IA (U-87 MG tumor-bearing mice) (n = 5), ¹⁸F-NODA-bivalent-IA (MDA-MB-231 breast tumor-bearing mice) (n = 3), and ¹⁸F-NODA-bivalent-IA coinjected with blocking dose of bivalent-IA (U-87 MG tumor-bearing mice) (n = 4).

excellent tumor uptake of $^{18}\text{F-bivalent-IA}$ in U-87 MG tumorbearing mice (3.69 \pm 0.62%ID/g), which was more than 4 times higher than that of MDA-MB-231 tumor-bearing mice (0.86 \pm 0.07%ID/g) (P < 0.001). Competition performed with $^{18}\text{F-bivalent-IA}$ and a block dose (6 nmol, 6 μg) of nonradioactive bivalent-IA decreased tumor uptake to 0.18 \pm 0.03%ID/g, which was approximately 20 times lower than mice imaged without cold compound (P < 0.0001). All biodistribution results in imaging and blocking study in different animal models had good correlation with semiquantitative ROI analysis of PET imaging studies.

In this study, we have successfully developed the first 18 F labeled non-peptidic bivalent integrin $\alpha_\nu\beta_3$ targeting radiotracer using a one step 18 F-AlF/NODA chelation reaction. The results demonstrate that 18 F-bivalent-IA is a highly potent and specific PET radiopharmaceutical to noninvasively image integrin $\alpha_\nu\beta_3$ in murine xenograft tumor models. Studies have shown the level of $\alpha_\nu\beta_3$ expression varies among individual cancer patients and high integrin $\alpha_\nu\beta_3$ expression has been correlated with disease progression and poor survival. $^{26-28}$ This new radiotracer, which can quantitatively visualize tumor integrin

expression by PET, has great potential for accurate cancer staging, patient selection for anti-integrin treatments, and therapy efficacy monitoring. Specially, ¹⁸F radiopharmaceutical is usually a time-consuming process with custom synthesis; the labeling procedures for the small molecule compound in this study is suitable to formulate into a lyophilized kit for ¹⁸F radiolabeling in the future. Further evaluation of safety and toxicology of ¹⁸F-bivalent-IA is ongoing.

ASSOCIATED CONTENT

S Supporting Information

Detailed methods of chemistry and radiolabeling of ¹⁸F-bivalent-IA, ELISA, cell uptake and blocking assay, small-animal PET imaging, biodistribution study, tumor tissue immunohistochemistry, and mouse serum stability study. This material is available free of charge via the Internet at http://pubs.acs.org.

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Notes

The authors declare no competing financial interest.

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