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# Detection of CrO<sub>4</sub><sup>2-</sup> Using a Hydrogel Swelling Microcantilever Sensor

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Hydrogels containing various mounts of tetraalkylammonium salts were used to modify microcantilevers for measurements of the concentration of CrO<sub>4</sub><sup>2-</sup> in aqueous solutions. These microcantilevers undergo bending deflection upon exposure to solutions containing various CrO<sub>4</sub><sup>2-</sup> concentrations as a result of swelling or shrinking of the hydrogels. The microcantilever deflection as a function of the concentration of  $CrO_4^{2-}$  ions is nearly linear in most concentration ranges. It was found that a concentration of 10<sup>-11</sup> M CrO<sub>4</sub><sup>2-</sup> can be detected using this technology in a fluid cell. Other ions, such as Br-, HPO<sub>4</sub><sup>2-</sup>, and NO<sub>3</sub><sup>-</sup>, have minimal effect on the deflection of this cantilever. The anions  $SO_4^{2-}$  and  $CO_3^{2-}$  could interfere with the CrO<sub>4</sub><sup>2-</sup> detection, but only at high concentrations ( $> 10^{-5}$  M). Such hydrogel-coated microcantilevers could potentially be used to prepare microcantilever-based chemical and biological sensors when molecular recognition agents are immobilized in the hydrogel.

Microcantilevers provide an outstanding platform for chemical and biological sensors because they have excellent dynamic response in a small package, with the opportunity to have integration of micromechanical components with on-chip electronic circuitry.<sup>1–12</sup> One unique characteristic of microcantilevers

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is their ability to undergo bending due to molecular adsorption or binding-induced change in surface tension. This is achieved by confining the adsorption to one side of the cantilever.<sup>6–8</sup> Microcantilever bending occurs in both air and solution. The key to microcantilever sensor development is to choose appropriate coatings for identification of chemically specific species. Two approaches have been used to immobilize the molecular recognition agents to the microcantilever surface. In the first approach, self-assembled monolayers have been proven successful for the detection of species in water,<sup>2–5</sup> while in the second, polymeric films, such as those developed for surface acoustic wave (SAW) devices, have been used for detection in the gas phase.<sup>6,7</sup> Recently, a polymer-coated microcantilever was also developed for measuring pH in solution.<sup>8</sup>

Chromium exists in the environment in different oxidation states in the groundwater, seawater, and soil.  $^{13}$  Cr(VI) in the form  $\text{CrO}_4{}^{2^-}$  is stable in neutral and alkaline environments, and it has been found to be very toxic to animals and humans.  $^{14}$  Accordingly, the development of methods for the detection of  $\text{CrO}_4{}^{2^-}$  in the environment is extremely important. Recently, we reported a  $\text{CrO}_4{}^{2^-}$  sensor based on a microcantilever modified with a self-assembled monolayer of a triethyl-12-mercaptododecylammonium salt.  $^5$  The surface-modified microcantilever sensor selectively responded to  $\text{CrO}_4{}^{2^-}$  with minimum interference from other anions, including  $\text{Cl}^-$ ,  $\text{CO}_3{}^{2^-}$ , and  $\text{SO}_4{}^{2^-}$ , etc. The detection limit of this sensor to  $\text{CrO}_4{}^{2^-}$  was  $10^{-9}$  M; however, the sensor gradually lost its sensitivity over one week because of the instability of the monolayer. Thus, the design of other coatings for the microcantilever is required for long-term monitoring purpose.

Stimuli—response hydrogels change volume in response to small changes in ionic strength, <sup>15</sup> solvent, <sup>16</sup> stress, <sup>17</sup> light intensity, <sup>18</sup> electric field, <sup>19</sup> and magnetic fields. <sup>20</sup> Such behavior has led

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to efforts to develop chemical and biological sensors for species such as glucose,  $^{21}$  Pb $^{2+},^{22}$  etc. The sensor platforms investigated to date include electrode,  $^{23}$  fluorescence,  $^{24}$  and crystalline colloidal array reflection.  $^{25}$  Taking advantages of the volume-changeable property of the hydrogel, we report here a hydrogel-coated microcantilever sensor for the detection of  $\text{CrO}_4{}^{2-}$ . (3-Acrylami-dopropyl)-trimethylammonium chloride (ATAC) was polymerized in a cross-linked hydrogel network as a result of its ability to form an ion pair with the  $\text{CrO}_4{}^{2-}$  anion following ion exchange from aqueous solution.

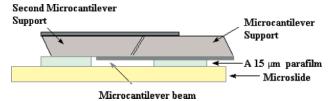
# **METHODS**

**1. Solvent and Materials.** We used commercially available silicon microcantilevers (Veeco Instruments, CA) in all of our experiments. The dimensions of the V-shaped microcantilevers were  $180~\mu m$  in length,  $25~\mu m$  in leg width, and  $1~\mu m$  in thickness. One side of the cantilever was covered with a thin film of chromium (3 nm) followed by a 20-nm layer of gold, both deposited by e-beam evaporation. The other side of the microcantilever was silicon with a thin naturally grown oxide layer.

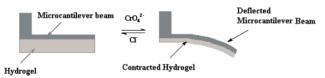
The chemicals used in these experiments, including  $Na_2CrO_4$ , NaCl, NaBr,  $Na_2CO_3$ ,  $NaHPO_4$ ,  $NaNO_3$ , allytriethoxysilane (ATS), MeOH, EtOH, (3-acrylamidopropyl)trimethylammonium chloride (ATAC), acrylamide (AMD), the cross-linker N,N-methylene-bis-(acrylamide) (bis-AMD), and the UV photoinitiator diethyoxyacetophenone (DEAP), were used as received from Aldrich. Highpurity deionized water was obtained with a Milli-Q water system (Millipore). The pH of the deionized water was 6.82. The pH of a  $10^{-3}$  M solution of NaCl was 7.0. The  $CrO_4^{2-}$ ,  $Br^-$ ,  $HPO_4^{2-}$ ,  $NO_3^-$ ,  $CO_3^{2-}$ , and  $SO_4^{2-}$  solutions used in our microcantilever deflection experiments were prepared in a  $10^{-3}$  M solution of NaCl. The pH of all these solutions was 7.0.

2. Polymerization Procedure. The precursor solution contained 2.1 mmol of AMD, 0.06 mmol of ATAC, 0.072 mmol of bis-AMD, and 0.0072 mmol of DEAP dissolved in 3 mL of water. A microcantilever was placed on a 1 cm<sup>2</sup> quartz microslide, separated from the quartz by a 15-µm Parafilm spacer. The microcantilever support was placed on the Parafilm spacer above the quartz surface so that there was a 15-µm distance between the microcantilever beam and the quartz microslide. The top and bottom sides of the microcantilever beams were gold and silicon surfaces, respectively. To prevent the exposure of the gold-coated surface to the solution, a second microcantilever was positioned to cover the gold-coated side of the first cantilever (Scheme 1). The quartz microslide was placed in the bottom of a vial that contained a precursor solution. The vial was cooled in an ice bath and then exposed to UV light from a 254-nm mercury lamp to initiate polymerization. After 12 min of exposure, the vial was removed

### Scheme 1



#### Scheme 2



from the UV light and the ice bath. The attachment of the hydrogel to the microcantilever silicon surface was observed by high-resolution optical microscopy. No hydrogel was attached on the gold surface, as observed using a microscope. The resulting hydrogel film bound to the substrate was exchanged and equilibrated in a  $10^{-3}$  M solution of NaCl for 1 day.

3. Deflection Measurement. The deflection experiments were performed in a flow-through glass cell (Digital Instruments, CA) such as that used in atomic force microscopy. The V-shape microcantilever was immersed in a 10<sup>-3</sup> M NaCl electrolyte solution. Initially, the NaCl solution was circulated through the cell using a syringe pump. A schematic diagram of the apparatus used in this study was previously reported.<sup>5</sup> Since a change in the flow rate induces noise in the cantilever bending signal due to turbulence, a constant flow rate of 4 mL/h was maintained during the entire experiment. Experimental solutions containing the base electrolyte and the anions of interest were injected directly into the slowly flowing fluid stream via a low-pressure injection port/sample loop arrangement. This arrangement allowed for continuous exposure of the cantilever to the desired solution without disturbing the flow cell or changing the flow rate. Since the volume of the glass cell, including the tubing, was only 0.3 mL, a relatively fast replacement of the liquid in contact with the cantilever was achieved.

Microcantilever deflection measurements by the optical beam deflection method were carried out with an AFM photodiode. The bending of the cantilever was measured by monitoring the position of a laser beam reflected from the cantilever onto a four-quadrant photodiode. The cantilever was immersed in the electrolyte solution until a stable baseline was obtained and the voltage of the position-sensitive detector was set as background corresponding to 0 nm. In our experiment, we define "bending down" as cantilever bending toward the silicon side while, "bending up" refers to bending toward the gold side.

## **RESULTS AND DISCUSSION**

A 15- $\mu$ m-thick layer of an ATAC copolymerized gel, coated on the surface of a microcantilever, was initially exposed to a constant flow (4 mL/h) of a  $10^{-3}$  M solution of NaCl. When solutions containing various concentrations of  $CrO_4^{2-}$  solutions were injected into the fluid cell, the microcantilever bent toward the gel side (silicon side) with different amplitudes as shown in Figure 1a. The microcantilever deflection increased as the concentration

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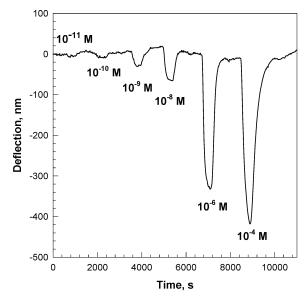
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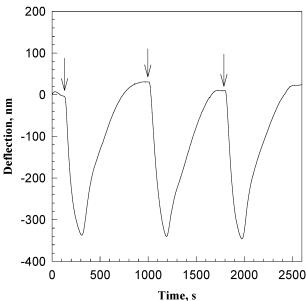


Figure 1. (a) Bending response as a function of time for a silicon microcantilever coated with a 15- $\mu$ m-thick layer of ATAC copolymerized hydrogel coated upon injection of different concentrations of  $CrO_4^{2-}$  solutions in 0.001 M NaCl background electrolyte solution. (b) Three replications of the bending response as a function of time following injection of a solution of  $10^{-6}$  M  $CrO_4^{2-}$  in 0.001 M NaCl solution (the injection point is indicated with arrows). Silicon microcantilever coated with a 15- $\mu$ m-thick ATAC copolymerized hydrogel.

of  $CrO_4^{2-}$  increased. For each measurement, a 0.5-mL aliquot of  $CrO_4^{2-}$  solution in  $10^{-3}$  M of NaCl was switched into the fluid cell, where the microcantilever was held. It took 7.5 min for the injected  $CrO_4^{2-}$  solution in  $10^{-3}$  M NaCl to flow through the fluid cell, and at this time, the original  $10^{-3}$  M NaCl solution was circulated back into the fluid cell. This correlates well with our observations that the deflection of the microcantilever reached a maximum  $\sim$ 7.5 min after the injection of various  $CrO_4^{2-}$  solutions. After this point, the microcantilever deflection gradually returned to its original position as the solution composition returned to the original  $10^{-3}$  M NaCl solution.

Repeated exposure of the same  $10^{-5}$  M solution of  $CrO_4^{2-}$  to the same cantilever modified with the hydrogel caused similar

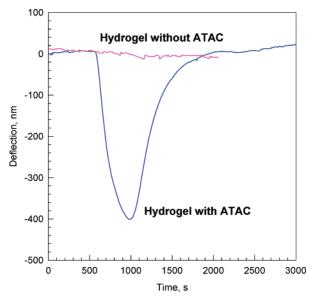


Figure 2. Bending response as a function of time, t, for silicon microcantilevers coated with hydrogel with and without ATAC component on the gold surface after injection of a solution of  $10^{-4}$  M CrO<sub>4</sub><sup>2-</sup> in 0.001 M NaCl. The microcantilevers were preequilibrated in the 0.001 M NaCl solution before injection of the CrO<sub>4</sub><sup>2-</sup> solution.

deflection amplitudes and bending rates, as shown in Figure 1b. The standard error is within 5%, indicating good measurement-to-measurement reproducibility.

Control experiments were performed with an unmodified microcantilever and using a microcantilever coated with a 15- $\mu$ m-thick hydrogel without the ATAC component. No deflection of the cantilever was observed upon exposure to a  $10^{-4}$  M solution of  $\text{CrO}_4^{2-}$ , as shown in Figure 2. Hydrogel film stability experiments were conducted on a microcantilever coated by an ATAC copolymerized hydrogel after 1 month and 2 months of storage in a 0.001 M NaCl solution. The cantilever deflection showed a similar profile and bending amplitude as those in Figure 2. This is a significant improvement in stability, as compared to the self-assembled monolayer-based microcantilever  $\text{CrO}_4^{2-}$  sensor that had been previously developed.

Figure 3 is a plot of the maximum deflection amplitude of a microcantilever coated with a tetraalkylammonium-containing hydrogel versus the concentration of CrO<sub>4</sub><sup>2-</sup>. The plot shows that this microcantilever can be used for the detection of CrO<sub>4</sub><sup>2-</sup> with a concentration as low as 10<sup>-11</sup> M in a solution with NaCl background electrolyte. The maximum bending of the microcantilever upon exposure to  $CrO_4^{2-}$  was  $\sim$ 400 nm. The effects of other anions, such as Br<sup>-</sup>, HPO<sub>4</sub><sup>2-</sup>, NO<sub>3</sub><sup>-</sup>, SO<sub>4</sub><sup>2-</sup>, and CO<sub>3</sub><sup>2-</sup>, on the deflections of the cantilever are also shown in Figure 3. Br<sup>-</sup>, NO<sub>3</sub><sup>-</sup> and HPO<sub>4</sub><sup>2-</sup>, SO<sub>4</sub><sup>2-</sup> and CO<sub>3</sub><sup>2-</sup> showed no effect on the cantilever when the concentrations of these anions were below 10<sup>-6</sup> M. At higher concentrations, NO<sub>3</sub><sup>-</sup>, HPO<sub>4</sub><sup>2-</sup>, and SO<sub>4</sub><sup>2-</sup> caused moderate cantilever deflections. The deflection at 10<sup>-4</sup> M was 110, 280, and 510 nm for  $NO_3^{2-}$ ,  $HPO_4^{2-}$ , and  $SO_4^{2-}$ , respectively. An  $\sim$ 700-nm deflection of the cantilever was observed when a 10<sup>-4</sup> M concentration of CO<sub>3</sub><sup>2-</sup> interacted with the hydrogel on the

Each point shown on the curve for  ${\rm CrO_4^{2-}}$  represents the mean  $\pm {\rm SE}$  from three independent determinations. The error induced

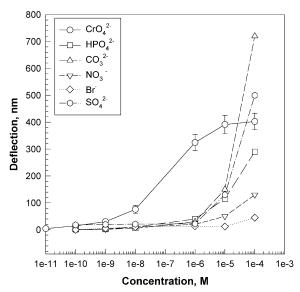


Figure 3. Maximum bending amplitude for a microcantilever coated with ATAC copolymerized hydrogel as a function of the change in concentration of  $\text{CrO}_4{}^{2-}$  and other anions.

by different microcantilevers was found to be within  $\pm 10\%$ . The data shows reasonably good reproducibility from cantilever to cantilever.

The results given above indicate that the hydrogel swells or shrinks upon ion exchange of  $CrO_4{}^{2-}$  or one of the other anions for  $Cl^-$ . The predominant Cr(VI) species under the experimental conditions of our experiments is  $CrO_4{}^{-2}$ . From the reported equilibrium constants for protonation of the chromate anion, extrapolated to infinite dilution,

$$HCrO_4^- \rightarrow CrO_4^{2-} + H^+$$

The measured p $K_a$  is 6.5 (25 °C),  $^{26}$  showing that the dianion predominates at pH 7. The pH-dependent dimerization equilibrium for chromate dianion,

$$2HCrO_4^- \leftrightarrow Cr_2O_7^{2-} + H_2O$$

has log K of 1.52 (25 °C, infinite dilution), <sup>26</sup> also confirming that at the concentrations under consideration in this work ( $<10^{-4}$  M), the chromate dianion predominates.

The expansion and contraction of gels allow chemical or electrical energy to be converted into mechanical work. Composite hydrogels have been well-studied over the past 30 years. We will adopt the standard hydrogel swelling theories elaborated by Flory<sup>27a</sup> and Tanaka<sup>27b</sup> to explain the volume change of the hydrogel upon exposure to  $\text{CrO}_4{}^{2-}$ . Recently, the hydrogel swelling upon interaction of specific analyte with receptors fixed to the hydrogel polymers has been intensively studied by Asher.<sup>28</sup>

In these theories, the equilibrium hydrogel volume is determined by the summation of three energies,

$$\Delta G_{\text{tot}} = \Delta G_{\text{mix}} + \Delta G_{\text{elas}} + \Delta G_{\text{ion}}$$
 (1)

where  $\Delta G_{mix}$  is the free energy of mixing of the polymer chains with the solvent medium,  $\Delta G_{elas}$  is the free energy of elasticity of the cross-linked network, and  $\Delta G_{ion}$  is the ionic electrostatic energy due to the Donnan equilibrium and electrostatic repulsions between charged side groups on the polymer backbone. Hydrogels that do not contain charged side groups on the polymer backbone do not change volume upon exposure to  $\text{CrO}_4{}^{2^-}$  in solution, as shown in the control experiment in Figure 2. This is consistent with the observations from Asher's group.<sup>28</sup>

As for the microcantilever modified with hydrogels that contain ATAC component, the downward bending of the microcantilevers suggests a shrinking of the hydrogel in response to the presence of  $\rm CrO_4^{2-}$  in the solution, as shown in Scheme 2. Figure 4 shows two pictures of an ATAC copolymerized hydrogel taken from a 0.001 M of NaCl solution and from a solution of  $10^{-5}$  M Na<sub>2</sub>CrO<sub>4</sub> in 0.001 M NaCl, respectively. The hydrogel contracted  $\sim\!30\%$  in response to the presence of  $\rm CrO_4^{2-}$  (based on the change in the longest dimension). Since most hydrogels are relatively homogeneous materials that shrink or swell uniformly, with no dramatic change in shape, the microcantilever bending is reversible and reproducible.

The maximum  $CrO_4^{2-}$  concentration in our experiments was at  $10^{-4}$  M, and the ionic strength changed  $\sim 30\%^{29}$  from a 0.001 M NaCl solution to a solution of  $10^{-4}$  M  $CrO_4^{2-}$  in 0.001 M NaCl. In all other  $CrO_4^{2-}$  solutions, the ionic strength differences with the 0.001 M NaCl electrolyte solution were <3%. The effect of such a small change in ionic strength on microcantilever bending can be neglected. Variation in pH can change the hydrogel volume. However, in our experiments, the pHs of all the solutions were 7.0, which argues against the pH effects on the hydrogel shrinking as an explanation for our observations. Thus, it appears that the observed ATAC copolymerized hydrogel shrinkage may be due primarily to an osmotic pressure decrease that arises from the ion exchange equilibrium of  $CrO_4^{2-}$  for chloride, ion-paired with the quaternary ammonium groups in the hydrogel, as shown in the following reaction.

$$CrO_4^{2-} + 2RN^+Me_3Cl^- \rightarrow (RN^+Me_3)_2 CrO_4^{2-} + 2Cl^-$$
 (2)

The ion pair formation between  $CrO_4^{2-}$  and the quaternary ammonium groups of a SAM-modified cantilever was postulated to be responsible for cantilever bending.<sup>5</sup> Prior to the introduction of  $CrO_4^{2-}$  into the solution in contact with the cantilever,  $Cl^-$  ions are associated with the quaternary ammonium cations. As illustrated in eq 2, the sorption of  $CrO_4^{2-}$  in solution requires two quaternary ammonium molecules in the hydrogel to maintain electrical neutrality. A smaller number of counter  $CrO_4^{2-}$  anions, one  $CrO_4^{2-}$  per two quaternary ammonium sites, are absorbed, causing the decrease of osmotic pressure from a Donnan-type potential and, subsequently, shrinking of the hydrogel. When the

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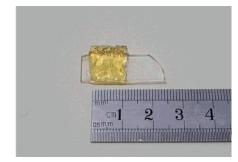


Figure 4. Pictures of an ATAC copolymerized hydrogel equilibrated with a 0.001 M NaCl solution for 2 days (left) and equilibrated with a solution of  $10^{-5}$  M Na<sub>2</sub>CrO<sub>4</sub> in 0.001 M NaCl overnight (right). The hydrogel on the right is yellow as a result of the absorption of  $CrO_4^{2-}$ . The transparent support is a quartz plate.

solution in contact with the hydrogel was replaced with NaCl, the quaternary ammonium ion pair converted back to  $R_4N^+Cl^-$ , which expanded the hydrogel.

Since the hydrogel film was relatively thick (15  $\mu$ m), it took hours for the whole film to reach the equilibrium in different  $CrO_4{}^{2-}$  solutions. To obtain a fast response, for each measurement in our experiments, a 0.5-mL buffer solution was injected into the fluid cell, and it took 7.5 min for the injected solutions to flow through the fluid cell, after which the original buffer solution was circulated back into the fluid cell. In consequence, only part of the ammonium groups in the polymer interacted with the  $CrO_4{}^{2-}$  in the solution, and the maximum response shown in Figures 1 and 2 did not provide a full picture of the microcantilever's actual response at equilibrium at each  $CrO_4{}^{2-}$  concentration.

The selectivity of this cantilever for  $CrO_4{}^2-$  over other anions can be explained  ${}^{5,31,32}$  by the hydration energy of  $CrO_4{}^2-$ . The hydration energy of  $CrO_4{}^2-$  is smaller than that of other anions, such as  $Br^-$ ,  $HPO_4{}^2-$ ,  $NO_3{}^-$ ,  $Cl^-$ , and  $CO_3{}^2-$ . These anions with higher hydration energies have a weaker association with the quaternary ammonium cation. After the  $CrO_4{}^2-$  solution is introduced, the  $Cl^-$  is displaced by stronger ion pair formation between  $CrO_4{}^2-$  and the quaternary ammonium cation. This explanation also provides an alternative, but equivalent, explanation for shrinking and swelling of the hydrogel layer that is more phenomenological in origin. Simply stated, the exchange of a highly hydrated anion, such as  $Cl^-$ , for a less hydrated anion, such as  $CrO_4{}^{-2}$ , contributes to a decrease in the volume of water within the pores of the hydrogel, leading to a decrease in the volume of the gel.  $^{31}$ 

Significant microcantilever bending that occurs following exposure to the divalent  $CO_3^{2-}$  and  $SO_4^{2-}$  anions at high

concentrations may be attributed to the smaller size of the  $CO_3^{2-}$  and  $SO_4^{2-}$ , as compared to  $CrO_4^{2-}$ . The radii of  $CrO_4^{2-}$ ,  $SO_4^{2-}$ , and  $CO_3^{2-}$  are 2.29, 2.18, and 1.89 Å, respectively.<sup>33</sup> The smaller 1:2 ion pair between  $CO_3^{2-}$  or  $SO_4^{2-}$  and tetraalkylammonium ions shrinks the hydrogel to a greater extent than  $CrO_4^{2-}$ . However, the higher threshold concentration of  $CO_3^{2-}$  or  $SO_4^{2-}$  reflects the greater selectivity of the quarternary ammonium modified hydrogel for  $CrO_4^{2-}$ .

#### CONCLUSIONS

Our study has shown that a hydrogel-modified cantilever can selectively respond to  $\text{CrO}_4{}^{2-}$  at concentrations as low as  $10^{-11}$  M. The sensitivity for detection of  $\text{CrO}_4{}^{2-}$  using a hydrogel-modified cantilever is much higher than the ISE method. Hydrogels, containing various molecular recognition receptors, could potentially be a general method for modification of the surface of microcantilevers for the detection of many chemical and biological species, because hydrogels have the property of converting chemical and electrical energy into mechanical energy.

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