

Tunable Aptamer Capillary Electrophoresis and Its Application to Protein Analysis

Hongquan Zhang, Xing-Fang Li, and X. Chris Le*

Department of Laboratory Medicine and Pathology, University of Alberta, Edmonton, Alberta, Canada T6G 2G3

Received October 14, 2007; E-mail: xc.le@ualberta.ca

Development of protein biomarkers for disease diagnosis and treatment requires the determination of multiple proteins that are present at trace levels. The sensitivity of the current assays for multiple proteins is often inadequate for detection of low-abundance proteins. Although affinity polymerase chain reaction,¹ affinity capillary electrophoresis,² proximity ligation,³ and nanotechnology⁴ have improved detection for specific proteins, these assays are usually applicable to a single protein at a time.

We describe here a tunable aptamer capillary electrophoresis assay enabling the ultrasensitive analysis of multiple proteins and protein isomers. The key concept is tuning the electrophoretic mobility of proteins with DNA aptamers to achieve efficient separation of multiple proteins or protein isomers. We introduce aptamers of varying nucleotide length as charge modulators to modify the electrophoretic mobility of proteins, tailored for the separation of the various protein-aptamer complexes in free solution. This systematic approach extends the applications of charge modulation in affinity assays⁵ and end-labeled free-solution electrophoresis of DNA.⁶

The principle of modulating the mobility of proteins may be expressed in the following equations, showing the dependence of electrophoretic mobility (μ) on the net charge (Z) and the mass (M) of the protein. In free-zone capillary electrophoresis, the electrophoretic mobility of a protein is proportional to its net charge, and inversely proportional to the frictional forces acting upon it in solution.⁷

$$\mu \approx C_p \frac{Z}{M^\alpha} \quad (1)$$

where C_p is a constant for a given protein, and α is a factor (0–1) describing the shape of the protein molecule. Upon the binding of an aptamer, the electrophoretic mobility of the protein is shifted to

$$\mu_c \approx C_p \frac{Z + n\Delta Z}{(M + n\Delta M)^\alpha} \quad (2)$$

where n is the number of nucleotides making up the aptamer, ΔZ is the change in charge per nucleotide, and ΔM is the change in size per nucleotide. Under the pH conditions (pH 7–9) typically used for capillary electrophoresis separation, ΔZ is nearly -1 owing to the phosphate group in the nucleotide and the effect of the counterions in solution.⁶ Because most proteins carry a small net charge,⁸ and the change in mass ΔM (~ 320 amu) per nucleotide is much smaller than the mass of a protein (M), the contribution of $n\Delta Z$ to the shift in mobility is often much more significant than that of $n\Delta M$. Therefore, eq 2 can be approximated to

$$\mu_c \approx C_p \left(\frac{Z}{M^\alpha} + \frac{n\Delta Z}{M^\alpha} \right) \quad (3)$$

Thus, the electrophoretic mobility of the proteins can be rationally controlled by modulating the length of the aptamer (n), taking into account the size of the protein (M), to achieve the desired value of the $n\Delta Z/M^\alpha$ term in eq 3.

To demonstrate the proof of principle, we first showed the tuning of mobility for the human immunodeficiency virus reverse transcriptase (HIV-RT) by binding it with a 49-nt aptamer, an 80-nt aptamer, and two 81-nt aptamers (Figure 1a). The aptamers, having a similar mass-to-charge ratio, migrate through the capillary at a similar mobility ($-2.81 \times 10^{-4} \text{ cm}^2 \text{ V}^{-1} \text{ s}^{-1}$). Upon binding of HIV-RT to the aptamers of varying length, the mobilities are shifted to -0.58×10^{-4} , -0.83×10^{-4} , and $-1.45 \times 10^{-4} \text{ cm}^2 \text{ V}^{-1} \text{ s}^{-1}$, respectively. An excellent linear association ($r^2 = 0.999$) between the mobilities of the three HIV-RT aptamer complexes (Figure 1a) and the length of aptamers supports the validity of eq 3. Similarly, the mobility of the thrombin-aptamer complexes shifted to $-2.22 \times 10^{-4} \text{ cm}^2 \text{ V}^{-1} \text{ s}^{-1}$ when using a full-length (76 nt) aptamer and further shifted to $-1.68 \times 10^{-4} \text{ cm}^2 \text{ V}^{-1} \text{ s}^{-1}$ when using a truncated (38 nt) aptamer (Figure 1b). Aptamers of different lengths can be made by maintaining the core sequence responsible for binding and either extending or truncating the aptamers at the ends. Thus, the mobilities of both large and small proteins (e.g., HIV-RT, 120 kDa; thrombin, 36 kDa) can be readily tuned using aptamers of appropriate length to achieve the desired separation.

Having achieved tunable mobility of proteins through their binding to tailored aptamers, we further applied the principle to the analysis of HIV-RT, thrombin, platelet derived growth factor (PDGF-BB), and human immunoglobulin E (IgE). Figure 2a shows a series of electropherograms from the analyses of these four proteins in mixture solutions containing varying concentrations of proteins (1–100 nM) and the corresponding aptamers for these proteins. The four protein-aptamer complexes are well resolved from one another and from the free (unbound) aptamers. Furthermore, adsorption of the basic proteins (IgE, $pI \approx 9.0$; PDGF-BB, $pI = 9.5$ – 10.5) on the negatively charged fused-silica capillary surface would have been a problem, if there were no aptamers binding to these proteins. The binding of the aptamers to the proteins makes the complex negatively charged, thereby eliminating the adsorption problem and focusing the protein-aptamer complexes into narrow zones. The ability to focus proteins and to tune their electrophoretic mobility using aptamers is the key to the successful analysis of multiple proteins using free zone capillary electrophoresis.

Another important benefit of aptamer binding to the proteins is the incorporation of fluorescent aptamers as probes to enable laser induced fluorescence (LIF) detection of proteins that are otherwise not amenable to high sensitivity LIF detection. We labeled the aptamers at the 5' end with highly fluorescent 6-carboxyfluorescein and excited it with an argon ion laser (488 nm). The binding of fluorescent aptamers to nonfluorescent proteins makes proteins amenable to highly sensitive LIF detection at 515 nm. Detection limits were 250 pM for IgE, 100 pM for HIV-RT and thrombin,

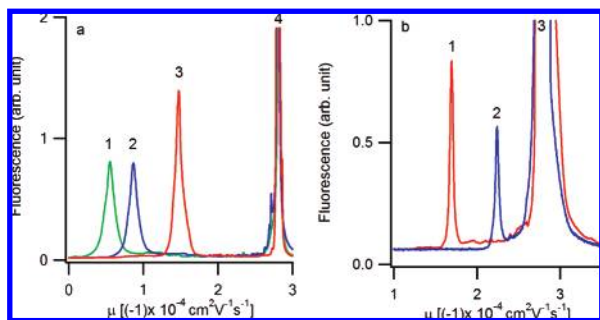


Figure 1. Electropherograms showing modulation of mobility of HIV-RT (a) and thrombin (b) by aptamers of variable lengths. (a) HIV-RT (10 nM) was incubated at 37 °C for 10 min with 100 nM of a 49-nt aptamer (green trace), an 80-nt aptamer (blue trace), and an 81-nt aptamer (red trace). Peak 1 corresponds to the complex of HIV-RT with the 49-nt aptamer, peak 2 is the complex of HIV-RT with the 80-nt aptamer, peak 3 is the complex of HIV-RT with two 81-nt aptamers, and peak 4 is the unbound (free) fluorescent aptamers. (b) Thrombin (25 nM) was incubated at 37 °C for 10 min with 100 nM of either a full-length aptamer (76 nt, blue trace) or a truncated aptamer (38 nt, red trace). Peak 1 is the complex of thrombin with the 38-nt aptamer, peak 2 is the complex of thrombin with the 76-nt aptamer, and peak 3 corresponds to the unbound fluorescent aptamers.

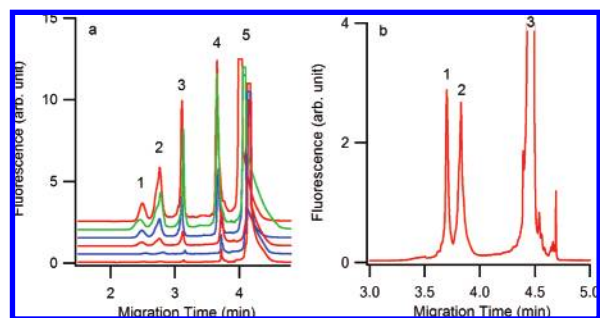


Figure 2. (a) Electropherograms showing the analysis of four proteins. Aptamer complexes of IgE (peak 1), HIV-RT (peak 2), thrombin (peak 3), and PDGF-BB (peak 4) are well resolved from the mixture of fluorescent aptamers (peak 5). The concentrations of proteins are 1, 5, 25, 50, 80, 100 nM from the bottom traces to the top, respectively. (b) Electropherograms showing the analysis of PDGF-AB and PDGF-BB isomers; 25 nM PDGF-AB and PDGF-BB were incubated at 37 °C for 10 min with 200 nM of a truncated 33-nt aptamer. Peak 1 is the complex of PDGF-AB with a single 33-nt aptamer, peak 2 is the complex of PDGF-BB with two 33-nt aptamers, and peak 3 is due to the unbound fluorescent aptamer.

and 50 pM for PDGF-BB. These are the best detection limits ever reported for the simultaneous determination of multiple proteins by capillary electrophoresis, recognizing that Dovichi and co-workers have demonstrated the detection of a single alkaline phosphatase enzyme molecule using a capillary electrophoresis enzyme assay.^{2d} Calibrations were linear for the determination of IgE ($r^2 = 0.991$), HIV-RT ($r^2 = 0.985$), thrombin ($r^2 = 0.984$), and PDGF-BB ($r^2 = 0.988$). A linear dynamic range of 2 orders of magnitude (1–100 nM in the low concentration region) was obtained for all four proteins, and this dynamic range could be extended to higher concentrations of proteins by using proportionally higher concentrations of aptamers.

To demonstrate the applicability of this assay to sample analysis, we spiked four proteins to 10-fold diluted human serum samples and determined the concentrations of the proteins in the spiked samples. Recoveries ranged from 92% to 113%. The analysis of the four proteins was complete in 5 min. Initial analysis of the serum samples showed matrix interference on the quantification of HIV-RT. We subsequently found that the addition of a nonspecific and nonfluorescent 49-mer oligonucleotide (sequence in Supporting Information, Table 1) could eliminate the interference, probably

by reducing any nonspecific binding of the serum proteins to the fluorescent aptamers.

Building on the success of separation and detection of the four proteins, we also applied the tunable aptamer capillary electrophoresis technique to the analysis of PDGF isomers, (Figure 2b). The sequences of PDGF A and B chains are ~60% identical, and the molecular weights of PDGF-AB (27 kDa) and PDGF-BB (25 kDa) are similar, making their separation difficult. However, using a 33-nt aptamer that binds to the B chain but not to the A chain of PDGF, we were able to tweak the electrophoretic mobilities of the PDGF isomers for their separation. As a result, PDGF-AB bound to a single aptamer is well resolved from PDGF-BB that is bound to two aptamer molecules (Figure 2b). To our knowledge, this is the first demonstration of the differentiation and detection of PDGF-AB and PDGF-BB isomers in a mixture by using an aptamer as a fluorescent probe.

In conclusion, we have developed a tunable aptamer capillary electrophoresis technique and demonstrated its application to the simultaneous determination of pM levels of four proteins in a single analysis. The principle was also applied to the separation and detection of two PDGF isomers. The multiplex capability and high sensitivity were accomplished by introducing tunable aptamers both as charge modulators for electrophoretic separation and as fluorescent affinity probes for ultrasensitive fluorescence detection. The assay is not limited to the four proteins shown here, and the principle can be extended to the simultaneous analysis of other species to which aptamers can bind, including proteins, peptides, carbohydrates, and whole cells. The throughput of the assay can be further enhanced by using electrophoresis systems with multiple capillaries⁹ or microfluidic devices with multiple channels. The assays for multiple proteins are potentially useful for biomarker development, clinical testing, and medical diagnostics.

Acknowledgment. This work is funded by NSERC Canada and National Natural Sciences Foundation of China.

Supporting Information Available: Detailed experimental procedures and the sequence of aptamers used in this study. This material is available free of charge via the Internet at <http://pubs.acs.org>.

References

- (1) (a) Sano, T.; Smith, C. L.; Cantor, C. R. *Science* **1992**, 258, 120–122. (b) Zhang, H.; Wang, Z.; Li, X.-F.; Le, X. C. *Angew. Chem., Int. Ed.* **2006**, 45, 1576–1580.
- (2) (a) German, I.; Buchanan, D. D.; Kennedy, R. T. *Anal. Chem.* **1998**, 70, 4540–4545. (b) Ostergaard, J.; Heegaard, N. H. H. *Electrophoresis* **2006**, 27, 2590–2608. (c) Berezovski, M.; Nutiu, R.; Li, Y.; Krylov, S. N. *Anal. Chem.* **2003**, 75, 1382–1386. (d) Craig, D. B.; Arriaga, E. A.; Wong, J. C. Y.; Lu, H.; Dovichi, N. J. *J. Am. Chem. Soc.* **1996**, 118, 5245–5253. (e) Wu, D.; Regnier, F. E. *Anal. Chem.* **1993**, 65, 2029–2035. (f) Yang, W.-C.; Schmitt, M. J.; Jackman, R.; Bodemer, W.; Yeung, E. S. *Anal. Chem.* **2005**, 77, 4489–4494. (g) Pavski, V.; Le, X. C. *Curr. Opin. Biotechnol.* **2003**, 14, 65–73.
- (3) Fredriksson, S.; Gullberg, M.; Jarvis, J.; Olsson, C.; Pietras, K.; Gustafsdottir, S. M.; Ostman, A.; Landergren, U. *Nat. Biotechnol.* **2002**, 20, 473–477.
- (4) (a) Nam, J. M.; Thaxton, C. S.; Mirkin, C. A. *Science* **2003**, 301, 1884–1886. (b) Hansen, J. A.; Wang, J.; Kawde, A.-N.; Xiang, Y.; Gothelf, K. V.; Collins, G. J. *Am. Chem. Soc.* **2006**, 128, 2228–2229.
- (5) (a) Yang, P.; Whelan, R. J.; Mao, Y.; Lee, A. W.-M.; Carter-Su, C.; Kennedy, R. T. *Anal. Chem.* **2007**, 79, 1690–1695. (b) Tim, R. C.; Kautz, R. A.; Karger, B. L. *Electrophoresis* **2000**, 21, 220–226.
- (6) Meagher, R. J.; Won, J.-I.; McCormick, L. C.; Nedelcu, S.; Bertrand, M. M.; Bertram, J. L.; Drouin, G.; Barron, A. E.; Slater, G. W. *Electrophoresis* **2005**, 26, 331–350.
- (7) (a) Gao, J.; Gomez, F. A.; Härter, R.; Whitesides, G. M. *Proc. Natl. Acad. Sci. U.S.A.* **1994**, 91, 12027–12030. (b) Gao, J.; Mammen, M.; Whitesides, G. M. *Science* **1996**, 272, 535–537.
- (8) Sear, R. P. J. *Chem. Phys.* **2003**, 118, 5157–5161.
- (9) Dovichi, N. J.; Zhang, J. Z. *Angew. Chem., Int. Ed.* **2000**, 39, 4463–4468.

JA0778747