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Abstract. Quantification of choroidal neovascularization (CNV) as visualized by optical coherence tomography angiography (OCTA) may have importance clinically when diagnosing or tracking disease. Here, we present an automated algorithm to quantify the vessel skeleton of CNV as vessel length. Initial segmentation of the CNV on *en face* angiograms was achieved using saliency-based detection and thresholding. A level set method was then used to refine vessel edges. Finally, a skeleton algorithm was applied to identify vessel centerlines. The algorithm was tested on nine OCTA scans from participants with CNV and comparisons of the algorithm's output to manual delineation showed good agreement. © The Authors. Published by SPIE under a Creative Commons Attribution 3.0 Unported License. Distribution or reproduction of this work in whole or in part requires full attribution of the original publication, including its DOI. [DOI: [10.1117/1.JBO.21.7.076010](https://doi.org/10.1117/1.JBO.21.7.076010)]

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1 Introduction

Age-related macular degeneration (AMD) is the leading cause of irreversible vision loss in older adults in the developed world.¹ The neovascular form of AMD is characterized by pathologic new vessels that grow from the choroid, through Bruch's membrane (BM), and into the avascular outer retina. There, the choroidal neovascularization (CNV) can cause sub-retinal hemorrhage, fluid exudation, or a number of other deleterious effects that negatively affect vision.² Fluorescein angiography (FA) and indocyanine green angiography are standard methods used to diagnose and evaluate CNV in the clinic. However, they are two-dimensional and require intravenous dye injection.

Optical coherence tomography (OCT) is a noninvasive imaging technique with micron-scale resolution that is commonly used in ophthalmology to assess retinal morphology. It is based on low-coherence interferometry and produces volumetric images composed of multiple depth-resolved reflectivity profiles. Optical coherence tomography angiography (OCTA) is a functional extension of OCT, which allows for the visualization of vasculature by assessing variation in the OCT signal over time. Regions with high variation represent motion from blood flow while regions with low variation represent static tissue. OCTA has generated significant clinical interest as a label-free method of angiography, and a number of recent studies have investigated its potential in visualizing CNV in AMD.^{3–7} Importantly, OCTA was shown to be able monitor changes in the CNV network over time in response to anti-vascular

endothelial growth factor (anti-VEGF) treatment.^{8–10} As a result, identification and quantification of the CNV network may have important clinical implications.

Despite rising interests, methods for automated detection and quantification of CNV are lacking. Often, quantification of CNV vessel area is subjective and relies on manual delineation.^{4,5} To address this issue, we previously developed a saliency-based detection algorithm, which could automatically separate the CNV membrane from noise/artifact on *en face* angiograms.¹¹ Within the detected CNV membrane, the CNV vessel area was quantified by thresholding to classify pixels as either vessel or noise/artifact and converting the pixel count to CNV vessel area. However, thresholding tended to preserve noise/artifact near vessel edges. More importantly, CNV vessel area gives greater weight to larger abnormal vessels, which may make it a less-sensitive metric to pruning/remodeling of smaller vessel as a result of anti-VEGF treatment.^{12,13} Thus, we sought to develop a level set method to segment neovascular vessels within the detected CNV membrane and a skeleton algorithm to determine vessel centerlines to quantify the vessel length of the CNV network.

2 Materials and Methods

2.1 Patient Selection and Data Collection

Participants diagnosed with neovascular AMD were recruited from the Casey Eye Institute Retina Service. Diagnosis was based on clinical presentation, a thorough examination, and an FA. Participants were enrolled after informed consent in accordance with an Institutional Review Board/Ethics Committee approved protocol at Oregon Health and Science University and in compliance with the Declaration of Helsinki.

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Two volumetric OCTA data sets were collected from the diseased eyes of nine participants using a commercial 70-kHz spectral domain OCT system with a center wavelength of 840 nm (Avanti RTVue XR, Optovue, Fremont, CA). The OCTA scan protocol for a single data set contained two sequential scans, each of which was acquired in less than 3 s and comprised of two repeated cross-sectional B-scans at 304 locations covering a 3×3 -mm area with a depth of 1.6 mm. Each B-scan was made up of 304 A-scans; each A-scan was 512 pixels in depth. The split-spectrum amplitude-decorrelation angiography (SSADA) algorithm was used to detect flow.^{14,15} Briefly, SSADA contrasts blood flow from static tissues by assessing the reflectance amplitude decorrelation on repeated B-scans at the same location. Split-spectrum processing was used to improve the signal-to-noise ratio of flow detection. For the first scan in the OCTA scan protocol, the fast scanning direction was in the transverse X -direction. For the second scan, the fast scanning direction was in the transverse Y -direction. The two orthogonal scans were then registered and merged to correct for motion from microsaccades and form a single data set.¹⁶

2.2 Algorithm Overview

The flowchart of the proposed algorithm is shown in Fig. 1. Following semiautomated segmentation to produce *en face* angiograms,¹⁷ the detection and quantification of the CNV network was achieved in four steps. First, the previously described saliency-based method was used to detect the CNV membrane. Second, thresholding was used to identify the initial CNV vascular region. Next, the CNV vasculature was refined using a level set method. Finally, a skeleton algorithm was used to locate the vessel centerlines. Sections 2.3–2.5 will describe the steps in more detail. The algorithm was implemented with custom software written in MATLAB® 2011a (MathWorks, Natick, MA).

2.3 Determining the Initial CNV Vascular Region

To visualize inner and outer retinal circulations, *en face* angiograms were constructed by maximum flow projection

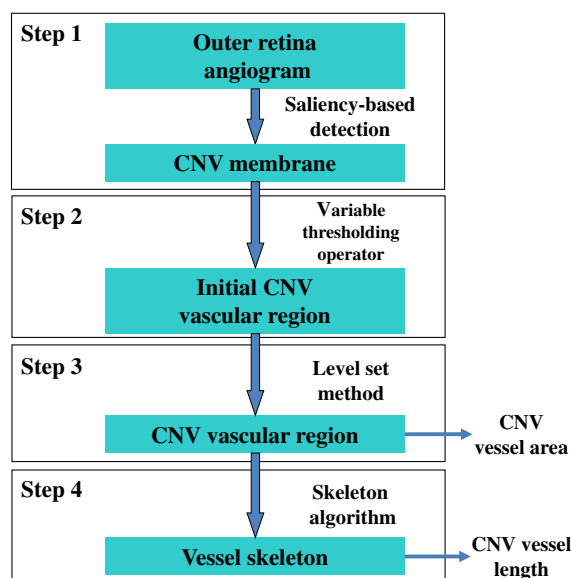


Fig. 1 Overview of the CNV vessel skeleton and quantification algorithm.

within slabs defined by segmented boundaries using semiautomated software.¹⁷ The inner retinal slab includes tissue layers between the inner limiting membrane and outer boundary of the outer plexiform layer (OPL), and the outer retinal slab includes layers between the outer boundary of OPL and BM.

In healthy eyes, the outer retina is typically avascular. However, OCTA suffers from shadowgraphic flow projection artifacts, whereby flow from superficial circulations can be replicated on deeper structures. Application of our previously developed saliency-based algorithm allowed for detection of the CNV membrane in the *en face* outer retinal angiogram.¹¹ Thresholding was then used to try and separate vessels from noise/artifact to generate the initial CNV vascular region. The threshold was set at two standard deviations above the mean decorrelation value in the foveal avascular zone.

2.4 Vascular Boundary Delineation

Thresholding tended to preserve noise/artifact near vessel edges. The flow signal within the initial CNV vascular region was thus inhomogeneous. We used a level set method with a local intensity clustering criterion to better separate the flow signal belonging to vessels from remaining noise/artifact.¹⁸ Image inhomogeneity could be described as

$$I = bJ + n, \quad (1)$$

where I is the measured flow signal in the outer retinal angiogram, J is the true signal, b is some bias field, and n is noise. The bias field represents scan and subject related variation in the OCTA signal caused by factors such as focus, aberrations, and attenuation from ocular media. Given an image $I: \Omega \rightarrow \mathbb{R}$, where Ω is a continuous domain, the aim was to segment the image into two disjoint regions Ω_i ($i = 1, 2$), where Ω_1 is the vessel region and Ω_2 is the background region. Let the terms x and y refer to pixels within the image. As the bias field b likely varied across the entire image, the separation of flow signal from noise/artifact was done in a circular neighborhood O_y centered at pixel y within Ω with a small radius ρ . Assuming b varied slowly, the value of b for some pixel x within O_y denoted as $b(x)$ could be approximated by a constant $b(y)$. The values $b(x)J(x)$ in each subregion can then be approximated by $b(y)c_i$, where c_i is an approximation of J and represents the detected flow signal in the vessel or background region. Standard K-means clustering was used to separate each pixel with $I(x) \approx b(y)c_i + n(x)$ for $x \in O_y$ as belonging to Ω_1 or Ω_2 based on iterative minimization of a clustering criterion function¹⁸

$$\varepsilon_y = \sum_{i=1}^2 \int_{\Omega_i} K(y-x) |I(x) - b(y)c_i|^2 dx, \quad (2)$$

where $b(y)c_i$ are the cluster centers to be optimized. $K(y-x)$ is a truncated Gaussian function, which gave larger weights to data closer to y and would equal 0 for $|y-x| > \rho$.

The above-defined local clustering criterion function classified the flow signal only within the circular neighborhood O_y . The integral of the local clustering criterion function ε_y for all y over the domain Ω constituted the overall function ε . The minimization of ε meant the joint minimization of ε_y for all y over the domain Ω and was done using a level set approach. In the level set method, ϕ was the level set function. The vessel

region was $\Omega_1 = \{x: \phi(x) > 0\}$ and the background region $\Omega_2 = \{x: \phi(x) < 0\}$. Their corresponding membership functions were defined as $M_i(\phi)$, where $M_1(\phi) = H(\phi)$ and $M_2(\phi) = 1 - H(\phi)$. H was a smoothed Heaviside function.¹⁹ The level set formulation was then as follows:¹⁸

$$\varepsilon(\phi, \mathbf{c}, b) = \int \sum_{i=1}^2 e_i(x) M_i[\phi(x)] dx, \quad (3)$$

where e_i is defined as

$$e_i(x) = \int K(y - x) |I(x) - b(y) c_i|^2 dy. \quad (4)$$

Two regularization terms were combined with $\varepsilon(\phi, \mathbf{c}, b)$ to generate the variational level set formulation as follows:

$$F(\phi, \mathbf{c}, b) = \varepsilon(\phi, \mathbf{c}, b) + \nu \cdot \int |\nabla H(\phi)| dx + \mu \cdot \int p(|\nabla \phi|) dx. \quad (5)$$

The second term on the right side of the equation computed the length of the zero level set function and was used to smooth the zero level set contour.¹⁹ The third term was the distance regularization term, and it was used to maintain the signed distance property during the level set evolution.^{20,21}

Pixel classification into Ω_1 or Ω_2 was achieved by minimizing the function F in an iterative process. A standard gradient descent approach based on the Gâteaux derivative $\partial F / \partial \phi$ was applied to minimize the function with respect to the variable ϕ for fixed \mathbf{c} and b . The gradient flow formulation was¹⁸

$$-\frac{\partial F}{\partial \phi} = \frac{\partial \phi}{\partial t} = -\delta(\phi)(e_1 - e_2) + \nu \cdot \delta(\phi) \cdot \operatorname{div} \left(\frac{\nabla \phi}{|\nabla \phi|} \right) + \mu \cdot \operatorname{div} [d_p(|\nabla \phi|) \nabla \phi]. \quad (6)$$

For fixed ϕ and b , the function was minimized with respect to \mathbf{c} as follows:

$$c_i = \frac{\int (b * K) I u_i dy}{\int (b^2 * K) I u_i dy}, \quad i = 1, 2, \quad (7)$$

where $u_i(y) = M_i[\phi(y)]$. Then, for fixed ϕ and \mathbf{c} , the function was minimized with respect to b as follows:

$$b = \frac{(IJ^{(1)}) * K}{J^{(2)} * K}, \quad (8)$$

where $J^{(1)} = \sum_{i=1}^2 c_i u_i$ and $J^{(2)} = \sum_{i=1}^2 c_i^2 u_i$.

In our implementation, the truncated Gaussian function $K(u)$ had a scale parameter $\sigma = 4$, and the mask size of the convolution kernel K was 17×17 . The radius ρ was then 8.5. Other parameters were as follows: $\tau = 1$ in the smoothed Heaviside function H_τ , the coefficient which modifies the first regularization term in Eq. (5) $\mu = 1$, $\nu = 0.001 \times 304^2$ which is a scale parameter that modifies the region size for the second regularization term in Eq. (5), and $\Delta t = 0.1$ for the gradient flow step size.

2.5 Vessel Skeleton and Quantification

The level set method separated vessels from background noise/artifacts to produce the CNV vascular region. This then allowed for the application of a skeleton algorithm on the binary image of the CNV vasculature. We used the Zhang–Suen²² parallel thinning algorithm and implemented it over a 3×3 pixel window. Briefly, the algorithm iteratively removes pixels until only a skeleton remains. In the first subiteration, south–east boundary and north–west corner pixels are considered. In the second subiteration, north–west boundary and south–east corner pixels are considered.

Quantification of CNV vessel area and vessel length was then performed on the binary image of the CNV vascular region and CNV skeleton, respectively. CNV vessel area was the sum of nonzero pixels converted to mm^2 . Vessel length was the sum of the pixels making up the skeleton converted to mm.

2.6 Verification of Results

The automated algorithm was applied to both OCTA scans from an eye, and within-visit repeatability was assessed using coefficient of variation. The CNV skeleton from the algorithm was compared to manual delineation of the CNV centerlines done by an experienced grader. The expert grader delineated the vessel centerlines of the CNV from the *en face* angiogram of the outer retinal slab. The grader had access to the inner retinal angiogram for reference. The Jaccard similarity metric was used to compare results from the automated algorithm and manual delineation:

$$J(I_a, I_m) = \frac{|I_a \cap I_m|}{|I_a \cup I_m|}, \quad (9)$$

where I_a is the result from the automated algorithm and I_m from manual delineation. However, due to the single pixel width of the skeletons, the union of results would be low. Thus, we broadened the centerlines from manual delineation using a dilation operator where the structure element was a disk with a radius of 1 pixel. I_b was the broadened skeleton from manual delineation. The Jaccard coefficient was between 0 and 1, with 1 denoting identity and 0 the complete dissimilarity. Errors rates were computed with the manually delineated vessel skeletons as the standard. False-positive error was the ratio of the total number of pixels in the algorithm-derived vessel skeleton that were not in the manually delineated vessel skeleton to the total number of pixels in the manually delineated vessel skeleton. False-negative error was the ratio of the total number of pixels in the manually delineated vessel skeleton that were not in the algorithm-derived vessel skeleton to the total number of pixels in the manually delineated vessel skeleton.

3 Results

The *en face* outer retinal angiogram from a participant with neovascular AMD was used as an example to show the workflow of the algorithm. Figure 2(a) shows the original outer retinal angiogram with CNV and projection artifacts. The CNV membrane [Fig. 2(b)] could be detected and extracted using a saliency-based approach.¹¹ We then used thresholding within the CNV membrane to generate the initial CNV vascular region shown [Fig. 2(c)]. The CNV vascular region contained noise/artifacts which would result in overestimation when quantifying CNV vessel area. The binary image of the CNV and its boundaries

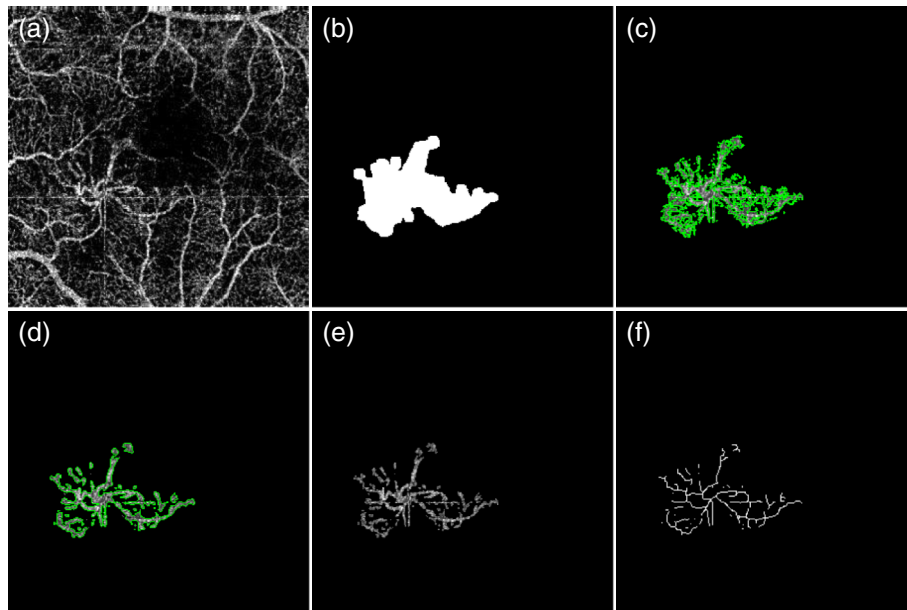


Fig. 2 The automated vessel skeleton algorithm. (a) Original outer retinal angiogram (3×3 mm) from a participant with neovascular AMD showing projection artifacts and CNV. (b) The CNV membrane obtained by saliency-based detection. (c) The CNV vascular region was contoured (green) and used to initialize the level set method. (d) The vessel boundaries segmented by the level set method. (e) The final CNV vascular region. (f) The vessel skeletons of the CNV.

[red contours in Fig. 2(c)] were used to initialize the level set method. The level set method iteratively performs the following: (1) estimate the flow signal in the vessel (c_1) and background (c_2) regions based on Eq. (7) (where u in the first iteration is the image used to initialize the level set method); (2) reclassify pixels as belonging to vessel or background based on Eq. (6); and (3) estimate the bias field (b) based on Eq. (8). After the level set function converged (c_i and b change becomes minimal), the final vessel boundaries were smooth and not surrounded by obvious noise/artifact [Fig. 2(d)]. The CNV vasculature shown in Fig. 2(e) was binarized and skeletonized. Figure 2(f) shows the vessel skeletons used to analyze the vessel length. The level set method and skeleton algorithm required 13 s to execute on an Intel Xeon CPU (E3-1226, 3.3 GHz); 93% of that time was spent on the level set evolution.

Data from nine participants with neovascular AMD were analyzed. Two volumetric data sets from each eye were evaluated to assess within-visit repeatability. Figures 3 and 4 show the results from one volumetric data set from the other eight participants. The cases included both type I and type II CNV with a wide range of sizes. Compared to determining CNV vessel area by thresholding, the level set method reduced the CNV vessel area measurement by $24.6 \pm 12.1\%$ (mean \pm standard deviation). The level set method improved within-visit repeatability, from a coefficient of variation of 7.3% with thresholding to 5.9%.

The skeleton algorithm was then applied to the initial CNV vascular region (thresholding vessel skeleton) and the output after level set evolution (level set vessel skeleton). The vessel skeleton results were compared to manual delineation of vessel centerlines. The level set vessel skeletons showed good agreement with manual delineation, with a Jaccard similarity metric of 0.69 ± 0.12 . This was an improvement (paired t -test $P < 0.001$) over thresholding vessel skeletons compared to

manual delineation, which had a Jaccard of 0.36 ± 0.07 . A comparison of false-positive and false-negative errors (Table 1) showed improvement in both with the level set approach ($P < 0.001$). A greater change was seen in the false-positive error metric, indicating that the level set method removed noise/artifact pixels to prevent an overly complex vessel skeleton. The vessel length within-visit repeatability as assessed with coefficient of variation was 1.8% for the level set vessel skeleton and 8.1% for manual delineation.

4 Discussion

OCTA is a relatively new approach to assessing CNV, and quantitative analysis of the CNV network may have important clinical implications. In this work, we developed a level set method to segment neovascular vessels and skeleton algorithm to determine vessel centerlines. The algorithm first identifies the CNV membrane using saliency-based detection. Next, thresholding is used to obtain the initial CNV vascular region. A level set method then refines the CNV vasculature, using local information to remove remaining noise/artifacts. Finally, a skeleton algorithm is applied to delineate the vessel centerlines based on the output from the level set method. The results of the algorithm as applied to nine eyes with neovascular AMD were shown. A comparison of the vessel skeleton from the algorithm to manual delineation showed good agreement with an average Jaccard similarity metric of 0.69.

Compared to thresholding when calculating CNV vessel area, the level set method reduced the value of the measurement by 24.6%. Inspection of the images showed that this reduction generally was removal of noise/artifact pixels near the edge of vessels. Unfortunately, it also removed pixels that may have been vessels with weak flow. For example (Fig. 5), in the participant shown in Fig. 2, there was removal of noise pixels near

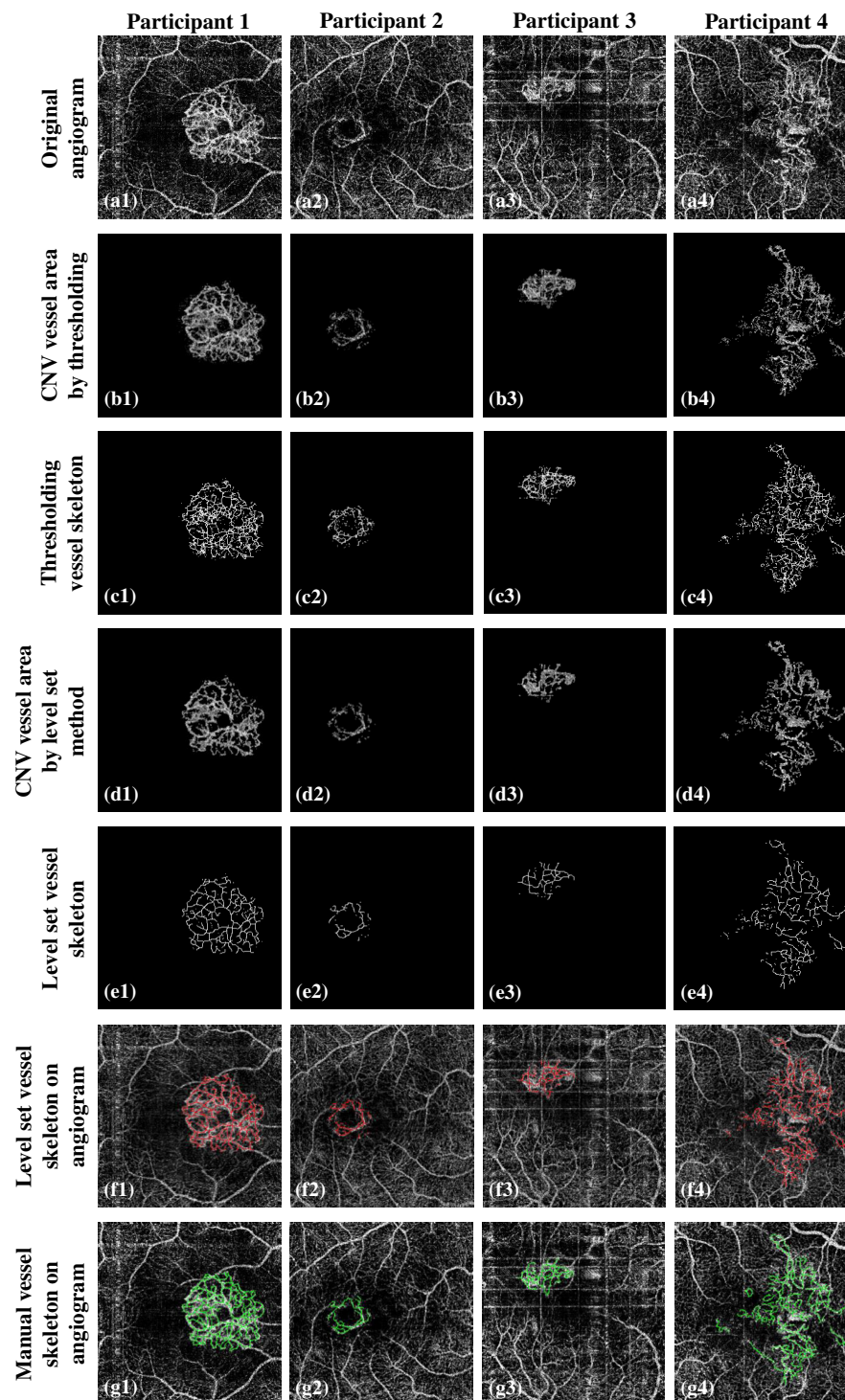


Fig. 3 Analysis of *en face* OCT angiograms from participants with neovascular AMD. The top row (a1)–(a4) shows the *en face* maximum flow projection angiogram from the outer retinal slab (3×3 mm) without any additional processing. The second row (b1)–(b4) shows the CNV following saliency-based detection and thresholding (b1) 0.943 mm^2 , (b2) 0.135 mm^2 , (b3) 0.245 mm^2 , (b4) 1.253 mm^2 . The third row (c1)–(c4) shows the vessel skeletons derived from the corresponding panel in (b): (c1) 31.549 mm , (c2) 6.493 mm , (c3) 9.967 mm , (c4) 37.934 mm . The fourth row (d1)–(d4) shows the CNV after the level set method (d1): (d1) 0.668 mm^2 , (d2) 0.129 mm^2 , (d3) 0.202 mm^2 , (d4) 0.804 mm^2 . The fifth row (e1)–(e4) shows the vessel skeletons derived from the corresponding panel in (d): (e1) 18.493 mm , (e2) 3.355 mm , (e3) 4.579 mm , (e4) 20.842 mm . The sixth row (f1)–(f4) shows the vessel skeletons in (e) on the original angiogram. The last row (g1)–(g4) shows the manually delineated vessel centerlines, which were used as the reference standard, on the original angiogram (g1) 21.355 mm , (g2) 3.622 mm , (g3) 5.477 mm , (g4) 23.743 mm .

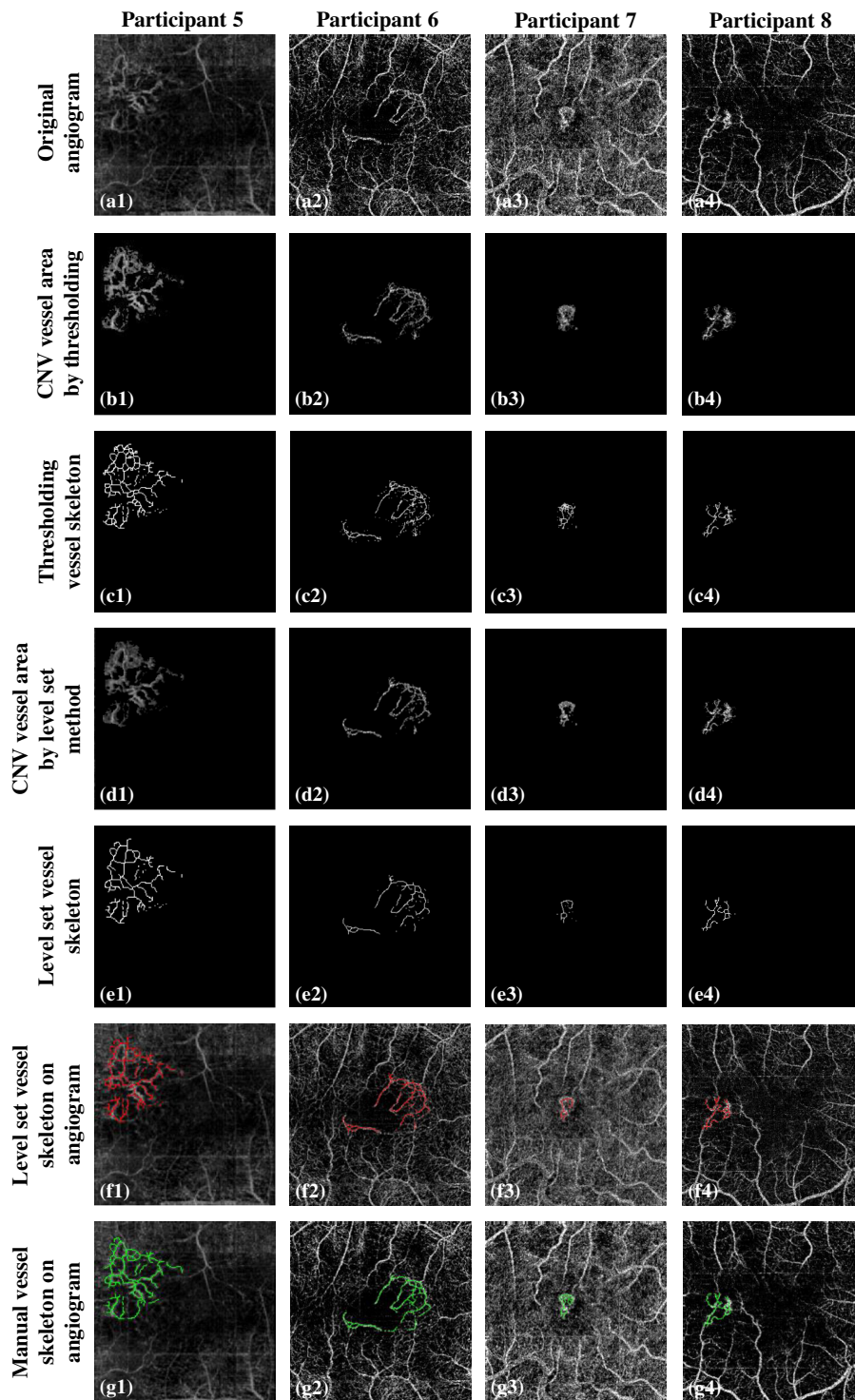


Fig. 4 Analysis of *en face* OCT angiograms from participants with neovascular AMD. The layout is the same as in Fig. 3. (b1) 0.855 mm²; (b2) 0.230 mm²; (b3) 0.088 mm²; (b4) 0.093 mm². (c1) 13.057 mm; (c2) 8.901 mm; (c3) 2.359 mm; (c4) 3.099 mm. (d1) 0.578 mm²; (d2) 0.191 mm²; (d3) 0.054 mm²; (d4) 0.066 mm². (e1) 9.800 mm; (e2) 5.763 mm; (e3) 1.066 mm; (e4) 2.388 mm. (g1) 10.329 mm; (g2) 6.375 mm; (g3) 1.411 mm; (g4) 2.625 mm.

Table 1 Agreement between automated algorithms and manual delineation of neovascularisation.

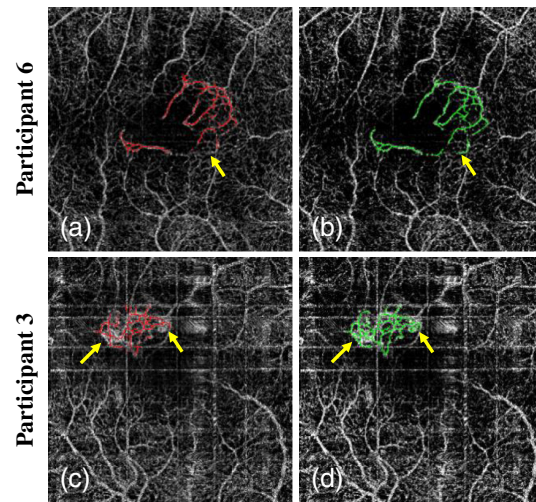
	Level set	Thresholding
Jaccard similarity metric	0.69 ± 0.12	0.36 ± 0.07
False-positive error	0.13 ± 0.07	0.90 ± 0.26
False-negative error	0.23 ± 0.10	0.34 ± 0.06

Mean \pm standard deviation of the Jaccard similarity metric and error rates were computed from the nine participants.

the edge of the CNV [green arrows in Figs. 5(b) and 5(c)], but also removal of vascular pixels within loops of the CNV network [yellow arrows in Figs. 5(b) and 5(c)]. A more quantitative evaluation of the impact of the level set method on CNV vessel area may prove insightful for future adjustments or modifications to the level set algorithm. Nevertheless, the application of the level set method to refine the CNV vasculature region simplified and improved the output from the skeleton algorithm [compare Figs. 5(d)–5(f)].

The CNV skeleton derived from skeletonization of the output from the level set method was generally comparable to manual delineation. Discrepancies occurred when the CNV detection missed parts of the CNV that had weak flow signal. For example, in participant 6, the grader drew vessels near the bottom of the CNV network [Figs. 6(a) and 6(b)] that were not included in the initial CNV vascular region [Fig. 4(b2)]. In addition, how the grader interpreted the vessel centerlines within a mass of flow signal did not always align with the algorithm output [Figs. 6(c) and 6(d)]. These issues suggest avenues for future improvement.

While the algorithm was capable of quantifying CNV vessel area and vessel length in the participants of this small study, additional studies with a larger number of diseased eyes are needed. Such a study would provide a better evaluation of the repeatability of the algorithm. Furthermore, it would be particularly insightful to test the algorithm's ability to detect changes in the CNV network as part of the natural progression of the disease or, alternatively, in response to treatment.

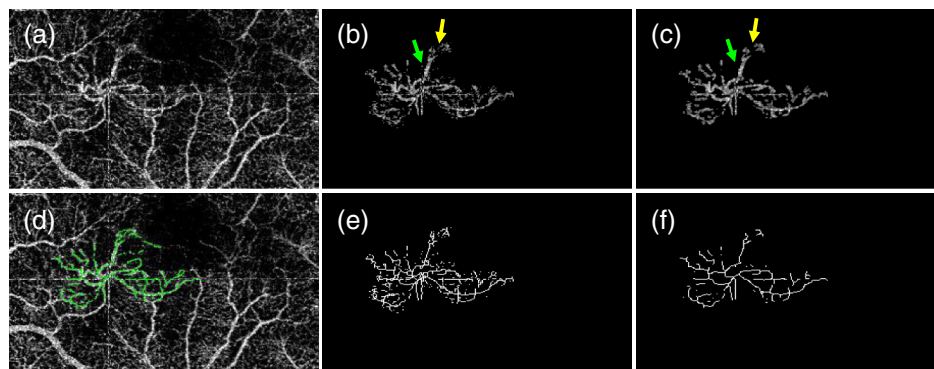
**Fig. 6** (a), (c) Comparison of the CNV skeleton from the automated algorithm and (b), (d) manual delineation. Arrows highlight discrepancies.

5 Conclusion

We developed an automated algorithm based on level set segmentation and skeletonization to delineate centerlines of CNV as visualized on *en face* OCT angiograms. Level set segmentation to refine CNV vessel edges preceding skeletonization was essential to improving the vessel skeleton output. CNV vessel skeleton results from the algorithm applied to OCTA scans from participants with neovascular AMD showed good within-visit repeatability and agreement with manual delineation.

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**Fig. 5** (a) Original angiogram. (b) CNV by thresholding. (c) CNV after level set evolution. Green arrows highlight removal of noise pixels near the edge of vessels. Yellow arrows show removal of vascular pixels with weak flow. (d) Manual delineation on the original angiogram. (e) The vessel skeleton output from the skeleton algorithm applied to (b) showing an overly complex skeleton. (f) The vessel skeleton output from the skeleton algorithm applied to (c).

also has a financial interest in Carl Zeiss Meditec. These potential conflicts of interest have been reviewed and managed by Oregon Health & Science University. Other authors do not have financial interest in the subject of this article.

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