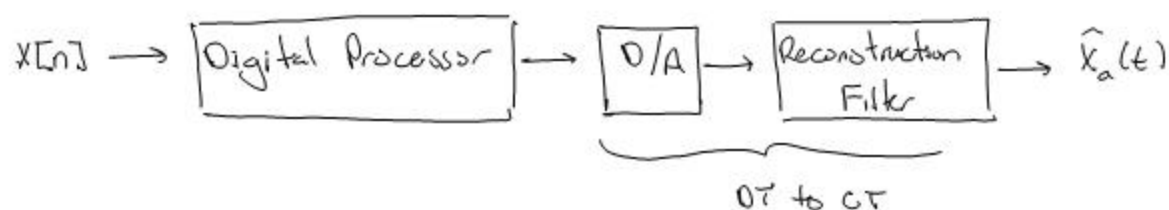
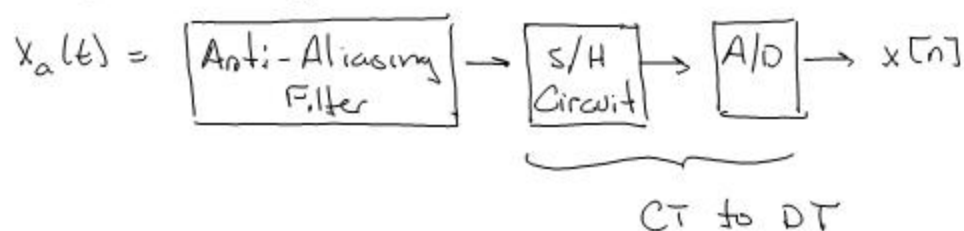


- Processing CT signals

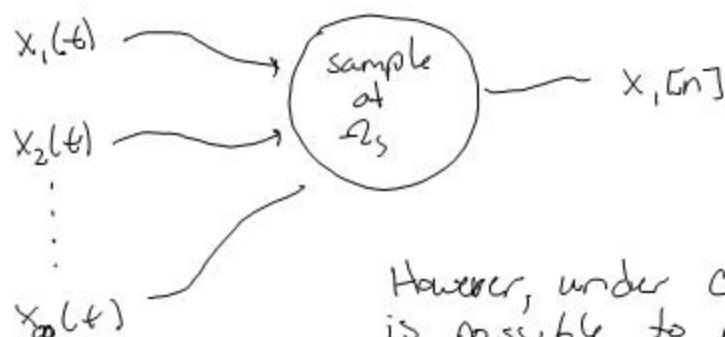


Questions:

- 1) What is the ideal sample rate?
- 2) What is the ideal anti-aliasing filter?
- 3) What is the ideal reconstruction filter?

- Sampling CT signals

Comment - In general, there exists an infinite number of CT signals, which when sampled at the same rate Ω_s result in the same DT signal.

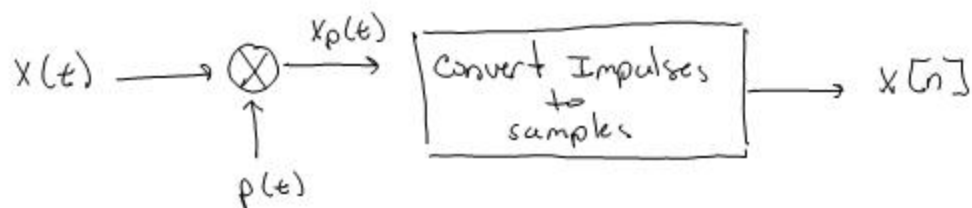


However, under certain circumstances, it is possible to relate a unique CT signal to a given DT sequence!

And... We can recover, exactly, the CT signal from the DT samples.

- CT signal sampling

- Multiplication by impulse train $p(t) = \sum_{n=-\infty}^{\infty} \delta(t - nT_s)$



$$x_p(t) = x(t)p(t) = x(t) \sum_{n=-\infty}^{\infty} \delta(t - nT_s) = \sum_{n=-\infty}^{\infty} x(t) \delta(t - nT_s)$$

$$= \sum_{n=-\infty}^{\infty} x(nT_s) \delta(t - nT_s)$$

The sample values $x(nT_s)$ weight the delta functions

We can extract the sample values by integration around each impulse.

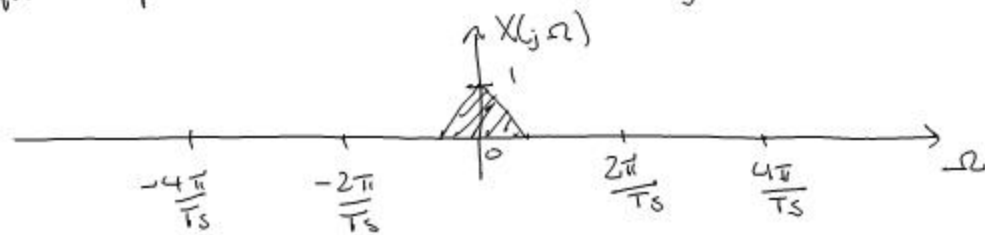
$$\int_{iT_s - \frac{T_s}{2}}^{iT_s + \frac{T_s}{2}} x_p(t) dt = \int_{iT_s - \frac{T_s}{2}}^{iT_s + \frac{T_s}{2}} \sum_{n=-\infty}^{\infty} x(nT_s) \delta(t - nT_s) dt$$

$$= \sum_{n=-\infty}^{\infty} x(nT_s) \int_{iT_s - \frac{T_s}{2}}^{iT_s + \frac{T_s}{2}} \delta(t - nT_s) dt$$

$$= \sum_{n=-\infty}^{\infty} x(nT_s) \delta(i - n) = x[i]$$

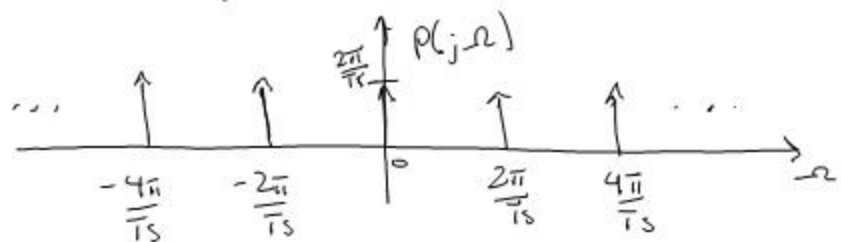
↑ sample value.

Suppose spectrum of $x(t)$ is $X(j\Omega)$ below -



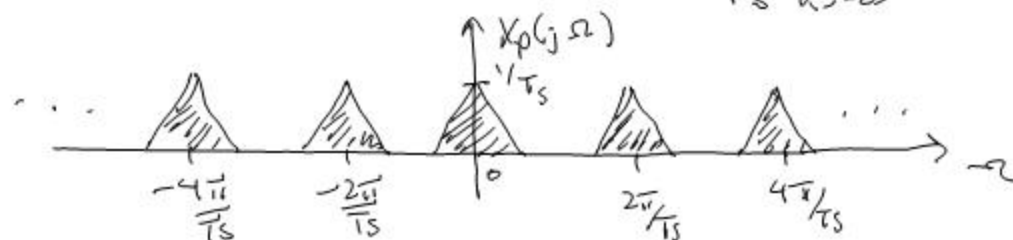
$$p(t) \xrightarrow{\text{CTFT}} P(j\Omega) = \Omega_s \sum_{k=-\infty}^{\infty} \delta(\Omega - k\Omega_s)$$

$$\text{Let } \Omega_s = \frac{2\pi}{T_s}$$



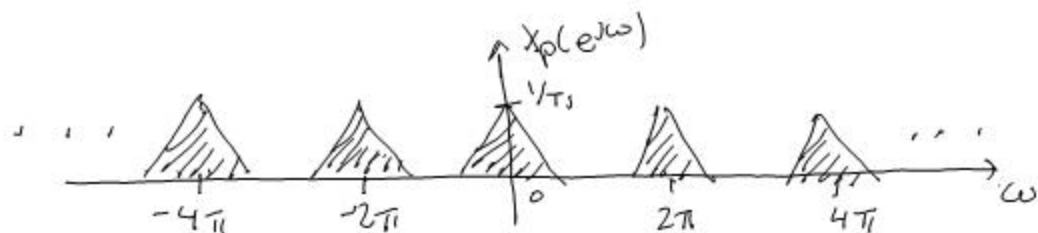
$$x_p(t) = x(t)p(t) \xrightarrow{\text{CTFT}} \text{Use modulation property}$$

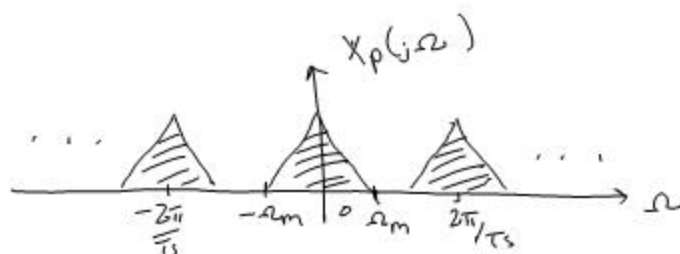
$$X_p(j\Omega) = \frac{1}{2\pi} X(j\Omega) * P(j\Omega) = \frac{1}{T_s} \sum_{k=-\infty}^{\infty} X(\Omega - k\Omega_s)$$



DTFT will look just like CTFT of $x_p(t)$ but frequency axis will be normalized.

$$\omega = \Omega T_s = \frac{\Omega}{F_s}$$





Notice - For no overlap in frequency domain replicas $\Omega_s > 2\Omega_m$. Overlap is called "aliasing". It is a form of distortion and is generally undesirable.

- CT recovery - If $\Omega_s \geq 2\Omega_m$, $x(t)$ can be recovered, exactly, from $x_p(t)$ by passing it through an ideal low pass filter with the following frequency response.

$$H_r(j\Omega) = \begin{cases} T_s & , |\Omega| \leq \Omega_c \\ 0 & , |\Omega| > \Omega_c \end{cases} \quad \text{where } \Omega_c \text{ is cutoff freq.}$$

Obviously, the cutoff freq, Ω_c should be greater than Ω_m but less than the lowest freq. of the next spectrum image, or replica.

Assume $\Omega_s = \frac{2\pi}{T_s}$, then $\Omega_m < \Omega_c < (\Omega_s - \Omega_m)$

Notice - The ideal reconstruction filter $H_r(j\Omega)$ has a gain of T_s .

- Ideal reconstruction filter impulse response

$$\begin{aligned} h_r(t) &= \frac{1}{2\pi} \int_{-\infty}^{\infty} H_r(j\Omega) e^{j\Omega t} d\Omega = \frac{T_s}{2\pi} \int_{-\Omega_c}^{\Omega_c} e^{j\Omega t} d\Omega \\ &= \frac{\sin(\Omega_c t)}{\Omega_c t/2} = \frac{\sin(\pi t/T_s)}{\pi t/T_s} \quad \text{for } \Omega_c = \frac{\pi}{T_s} \end{aligned}$$

- Reconstructed CT signal

$$\hat{x}(t) = h_r(t) * x_p(t)$$

$$= \frac{\sin(\pi t/T_s)}{\pi t/T_s} * \sum_{n=-\infty}^{\infty} x(nT_s) \delta(n - nT_s)$$

$$= \sum_{n=-\infty}^{\infty} x(nT_s) \frac{\sin(\pi(t - nT_s)/T_s)}{\pi(t - nT_s)/T_s}$$

Thus, $\hat{x}(t)$ is found by interpolating in between the sample values $x(nT_s)$ using the sinc function.

- Sampling terminology

$\Omega_s \geq 2\Omega_m$ "Nyquist condition"

Ω_m "Nyquist frequency"

$2\Omega_m$ "Nyquist Rate"

$\Omega_s > 2\Omega_m$ "oversampling"

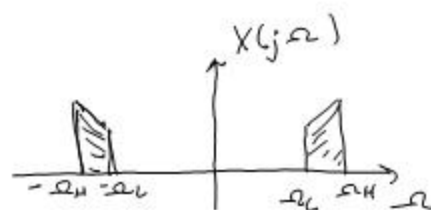
$\Omega_s < 2\Omega_m$ "under sampling"

$\Omega_s = 2\Omega_m$ "critical sampling"

- Bandpass sampling

$$\Omega_L \leq |\Omega| \leq \Omega_H$$

$$B = \Omega_H - \Omega_L \quad \text{"Bandwidth"}$$



Method 1 - Frequency shift to baseband, LP filter, sample at $\Omega_s \geq 2B$.

Method 2 - Sample at $\Omega_s \geq 2\Omega_H$.

Method 3 - Bandpass sample

Assume $\Omega_H = mB$ and choose $\Omega_s = 2B = \frac{2\Omega_H}{m}$
where $m > 1$.

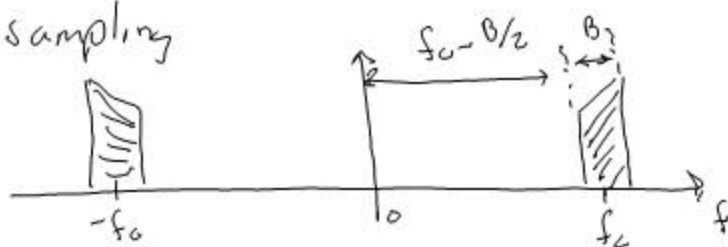
After sampling (multiplication by impulse train) -

$$X_p(j\Omega) = \frac{1}{T} \sum_{k=-\infty}^{\infty} X_a(j(\Omega - 2k\Omega_s))$$



Q: What if $\Omega_H \neq mB$

- More general bandpass sampling



$$\frac{m f_s}{2} = f_c - B/2$$

$$\Rightarrow f_s = \frac{2f_c - B}{m}$$

where $m > 0$, but $f_s \geq 2B$!

- Band pass sampling cont.

In fact - $f_s \leq \frac{2f_c - B}{m}$

and

$$f_s \geq \frac{2f_c + B}{m+1}$$

$$\Rightarrow \frac{2f_c - B}{m} \geq f_s \geq \frac{2f_c + B}{m+1}$$

- Filtering Concept - Pass certain frequencies of an input signal without distortion and block other frequencies.

$$H(e^{j\omega}) = |H(e^{j\omega})| e^{j\phi(\omega)}$$

↑ design this to attenuate or gain certain frequencies.

Low Pass Example -

$$|H(e^{j\omega})| \cong \begin{cases} 1, & 0 \leq |\omega| \leq \omega_c \\ 0, & \omega_c < |\omega| < \pi \end{cases}$$

If input is $x[n] = A \cos(\omega_1 n) + B \cos(\omega_2 n)$
and $\omega_1 < \omega_c$, $\omega_2 > \omega_c$ -

Output is $y[n] \approx A |H(e^{j\omega_1})| \cos(\omega_1 n + \phi(\omega_1))$

- Phase Delay - single frequency component

Input: $x[n] = A \cos(\omega_0 n + \phi)$

Output: $y[n] = A |H(e^{j\omega_0})| \cos(\omega_0 (n + \frac{\theta(\omega_0)}{\omega_0}) + \phi)$

$$\tau_p(\omega_0) = -\frac{\theta(\omega_0)}{\omega_0} \quad \text{"phase delay"}$$

- Group delay - when input is superposition of many sinusoidal components, not harmonically related -

Each component has a different phase delay -

$$\tau_g(\omega) = -\frac{d\theta(\omega)}{d\omega} \quad \text{"group delay"}$$