

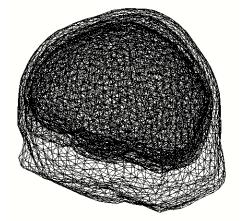


EEG/MEG 2:Head and Forward Modelling Olaf Hauk

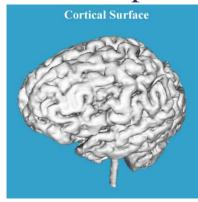
olaf.hauk@mrc-cbu.cam.ac.uk

Ingredients for Source Estimation

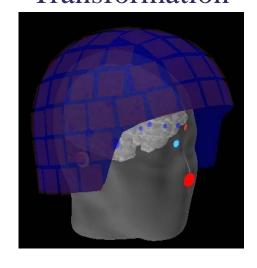
Volume Conductor/ Head Model



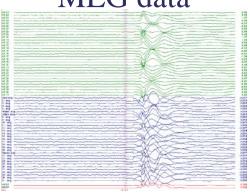
Source Space



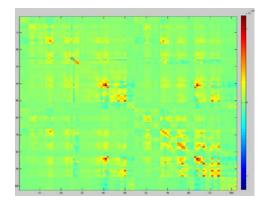
Coordinate Transformation



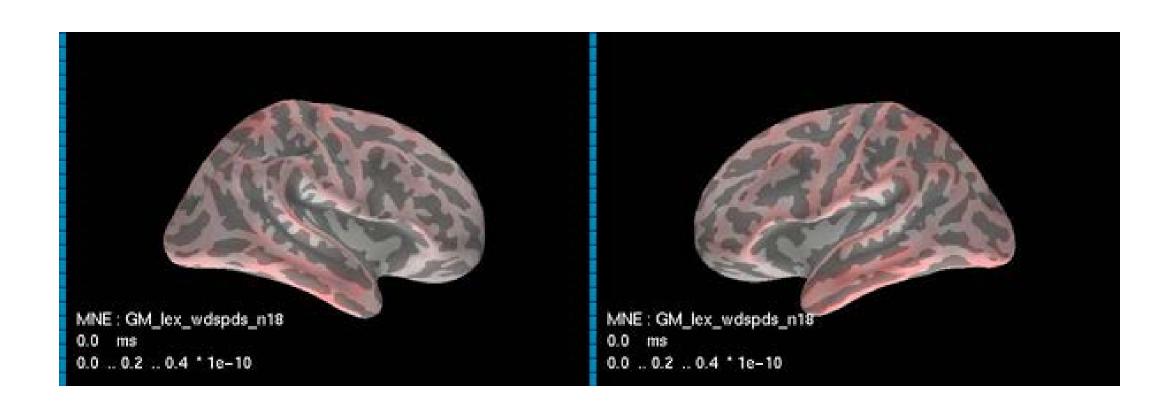
MEG data



Noise/Covariance Matrix

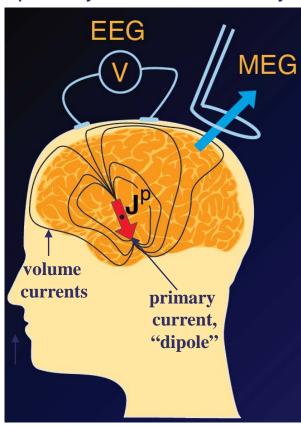


Our Goal: Spatio-Temporal Brain Dynamics "Brain Movies"



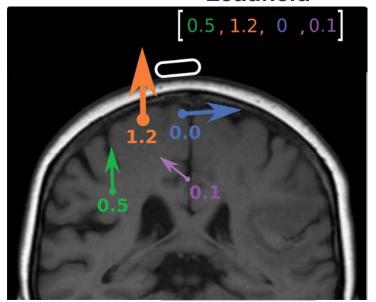
We Have To First State The Forward Problem In Order To Solve The Inverse Problem

EEG/MEG measure the primary sources indirectly



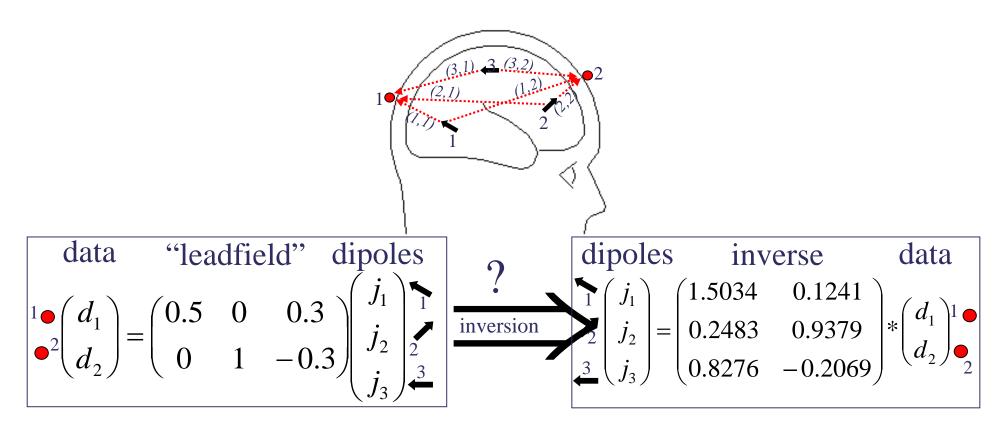
Sensors are differently sensitive to different sources

"Leadfield"



Hauk, Strenroos, Treder. In: Supek S, Aine C (edts), "Magnetoencephalography: From Signals to Dynamic Cortical Networks, 2nd Ed."

The EEG/MEG Forward Problem

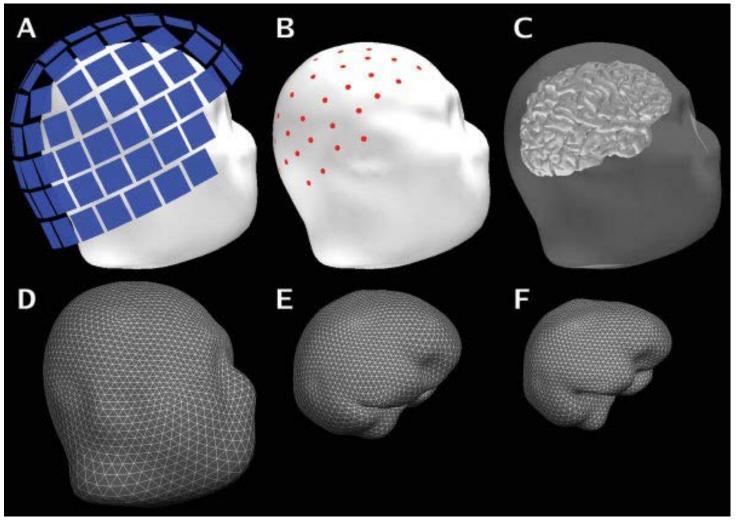


 $j_1 + j_2 = 1$ under-determined problem, no unique solution

d=Lj

d: data (n_sensors x 1) **L**: "leadfield" (n_sensors x n_dipoles), **j**: dipoles (n_dipoles x 1) Usually n_dipoles >> n_sensors.

Ingredients for a head model

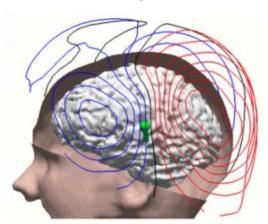


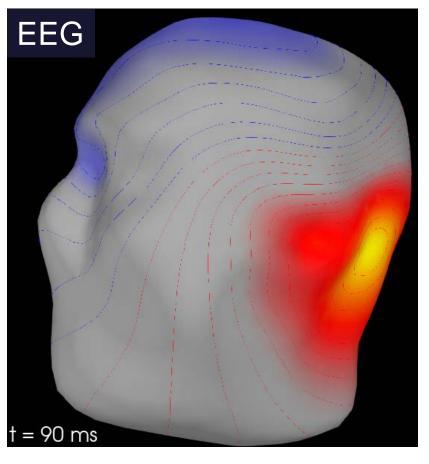
Goldenholz et al., HBM 2009 https://pubmed.ncbi.nlm.nih.gov/18465745/

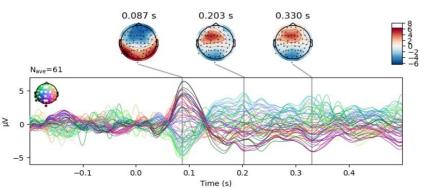
If you don't have individual MRIs: Standard head models and spherical approximations are available.

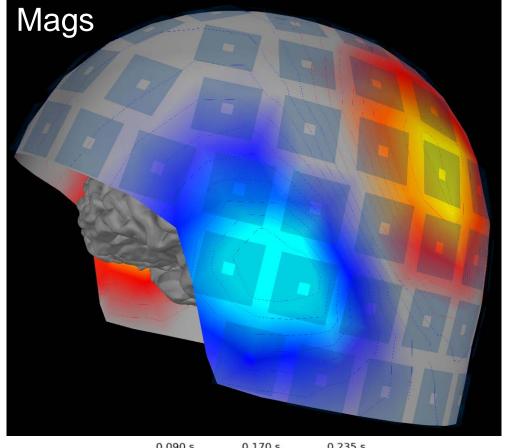
Example: Auditorily Evoked Activity

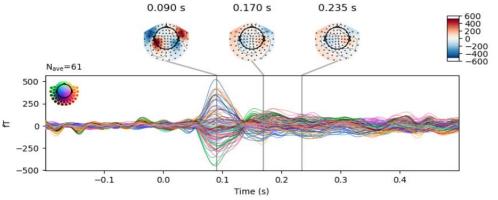
Tone to right ear





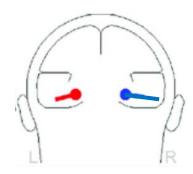


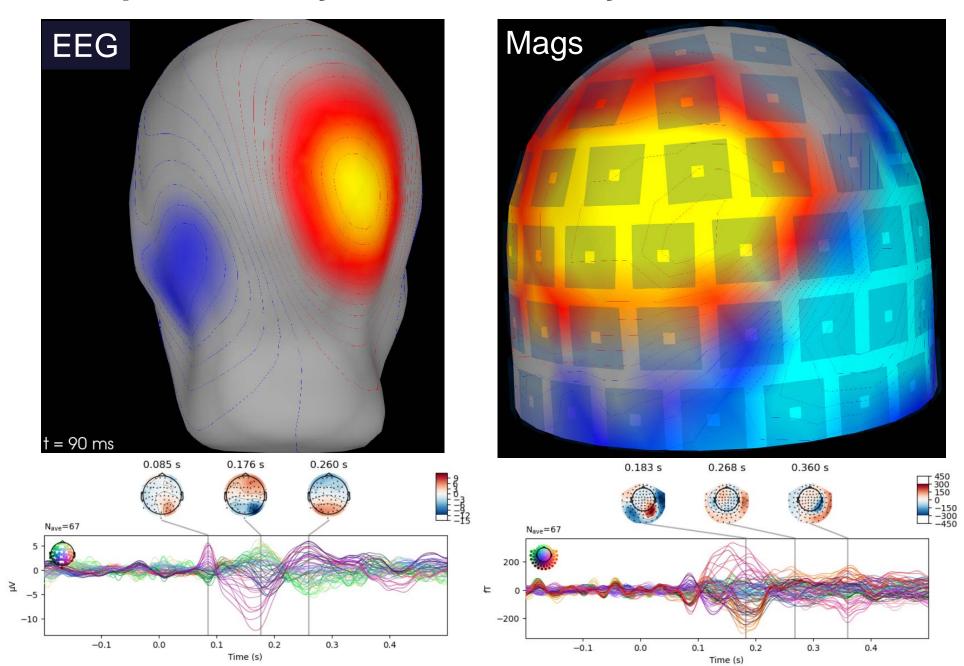




Example: Visually Evoked Activity ~100 ms

Checkerboard to left visual field



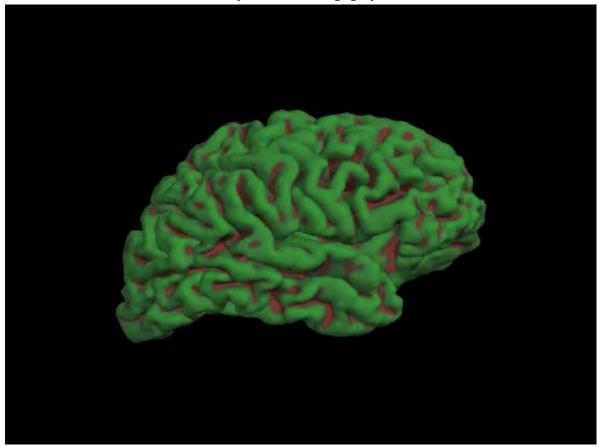


The Forward Problem and Head Modelling

Source Spaces

Source Space

Where active sources may be located, e.g. grey matter, 3D volume



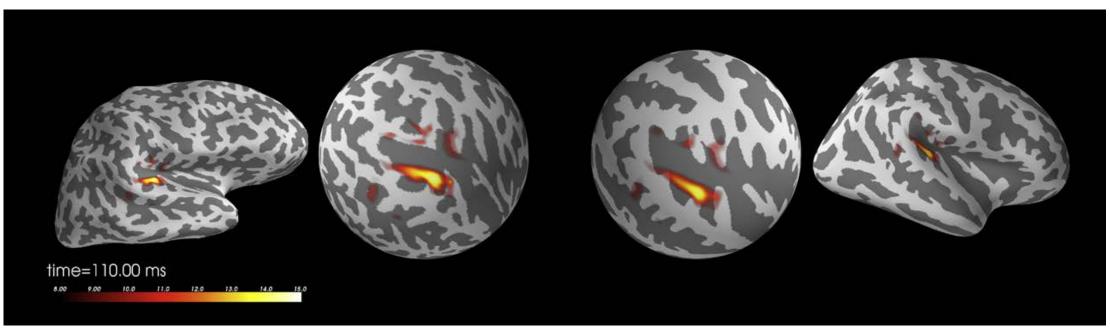
http://www.cogsci.ucsd.edu/~sereno/movies.html

Sometimes "standard head models" are used, when no individual MRIs available.

SPM uses the same "canonical mesh" as source space for every subjects, but adjusts it individually.

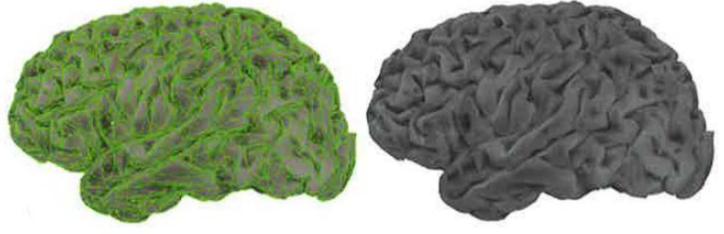
Normalising (Morphing) Cortical Surfaces

Morphing from individual to standard brain

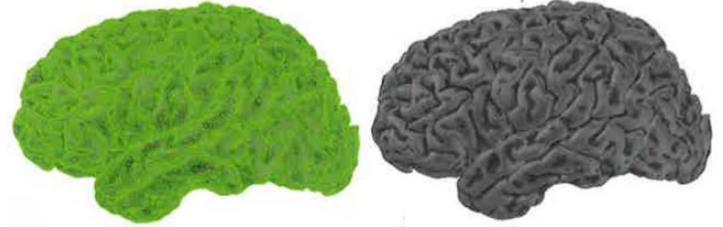


Spatial Sampling of Cortical Surfaces

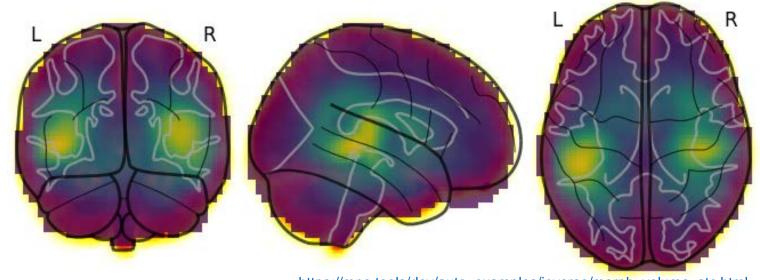
10.034 vertices, 20.026 triangles of 10 mm² surface area Sufficient for most EEG/MEG applications



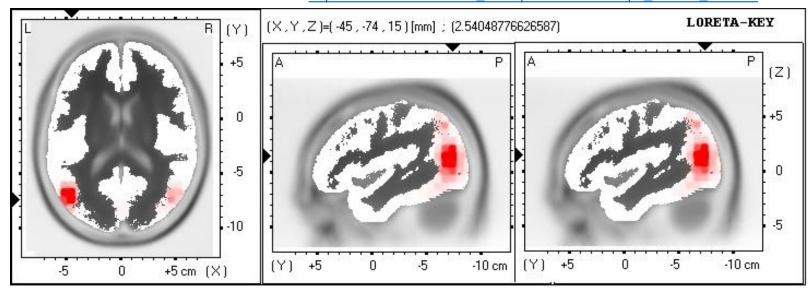
79.124 vertices, 158.456 triangles of 1.3 mm² surface area



Volumetric Source Spaces Are Possible



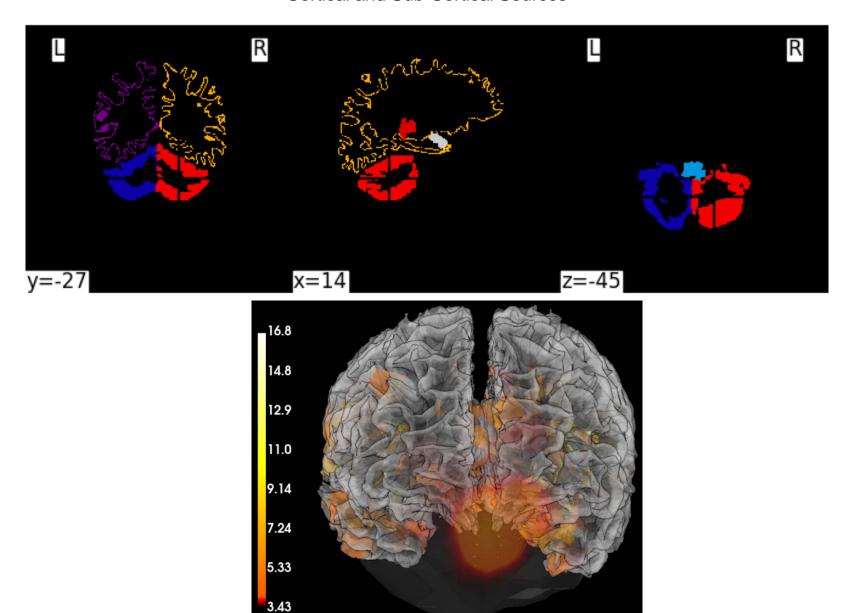
https://mne.tools/dev/auto_examples/inverse/morph_volume_stc.html



Pascqual-Marqui, PTRS-A 2011

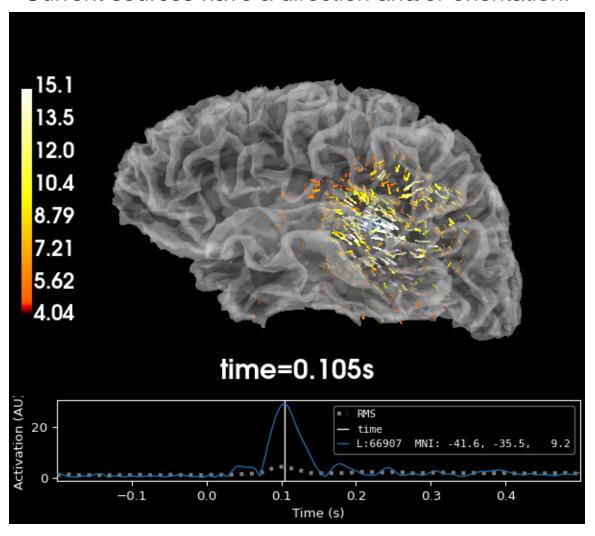
Mixed Source Spaces

Cortical and Sub-Cortical Sources

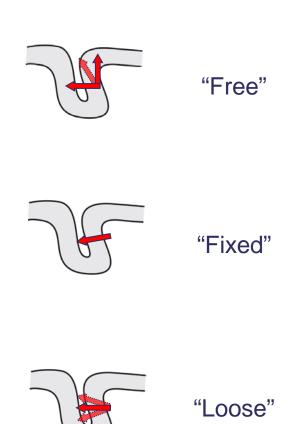


Source Orientations

Current sources have a direction and/or orientation.

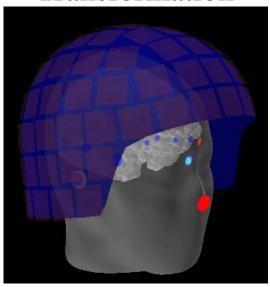


Constraints on source orientation:

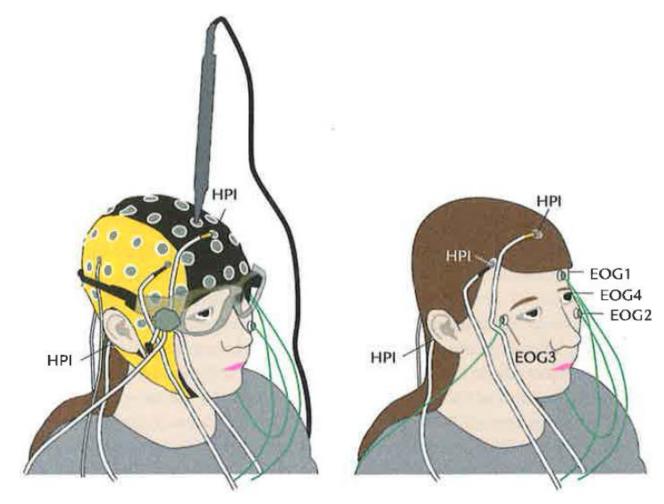


Coregistration of EEG/MEG and MRI Spaces

Coordinate Transformation



Coregistration of EEG/MEG and MRI Spaces

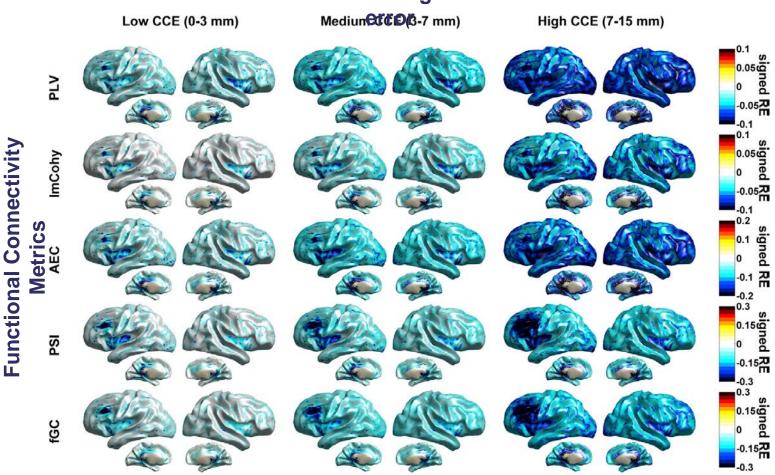


MNE-Python tutorial: https://www.youtube.com/watch?v=ALV5qqMHLIQ

Accurate Coregistration Is Important

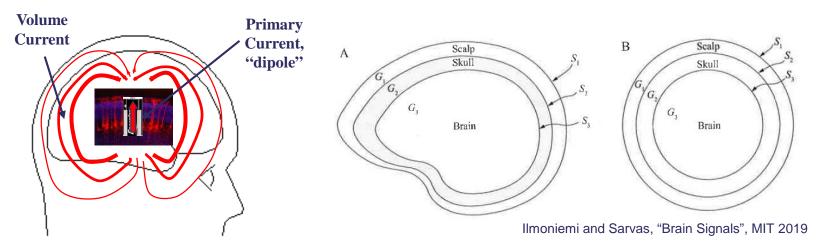
Coregistration errors affect the forward model, and therefore everything that follows.

For example, connectivity analysis: 3 levels of coregistration

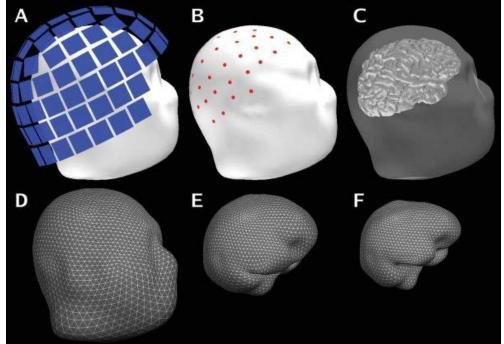


Head Models

Boundary Element Model (BEM)

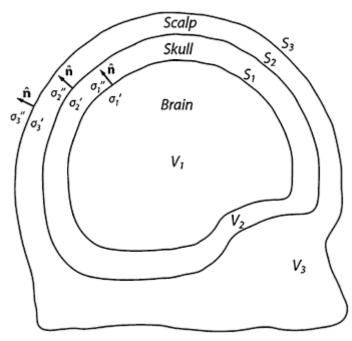


Ingredients for a head model



Goldenholz et al., HBM 2009

Boundary Element Model (BEM)



$$\sigma(\mathbf{r}) V(\mathbf{r}) = \frac{1}{4\pi} \sum_{j} \left(\sigma'_{j} - \sigma''_{j} \right) \int_{S_{j}} dS'_{j} \mathbf{n} \left(\mathbf{r}' \right) \cdot \frac{\mathbf{r}' - \mathbf{r}}{\left| \mathbf{r}' - \mathbf{r} \right|^{3}} V(\mathbf{r}')$$
$$+ \frac{1}{4\pi} \int_{V} d^{3}r' \mathbf{J}^{\mathbf{p}} \left(\mathbf{r}' \right) \cdot \frac{\mathbf{r} - \mathbf{r}'}{\left| \mathbf{r}' - \mathbf{r} \right|^{3}}.$$

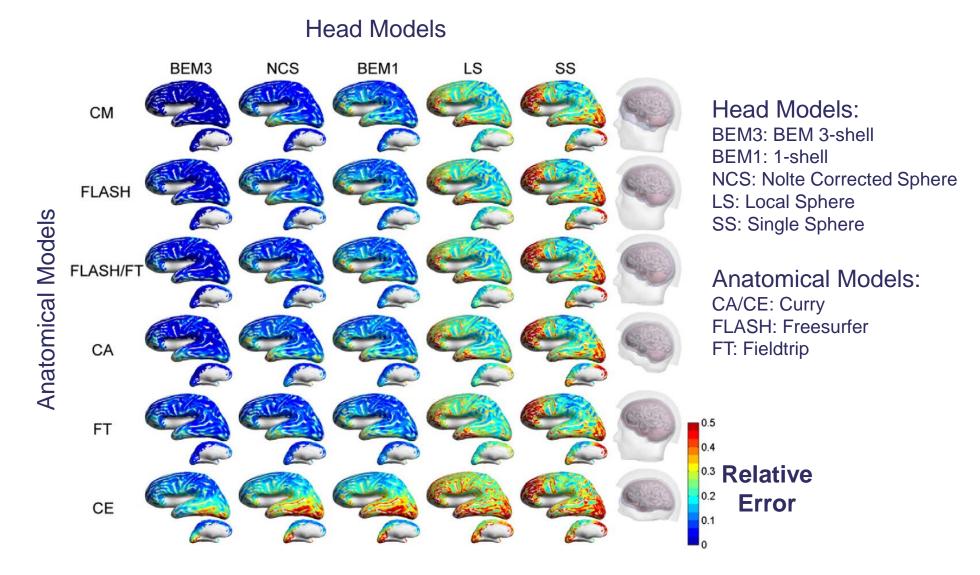
Magnetic Field

$$\begin{split} \mathbf{B}^{\mathbf{p}}\left(\mathbf{r}\right) &= \frac{\mu_{0}}{4\pi} \int_{V} \mathbf{J}^{\mathbf{p}}\left(\mathbf{r}'\right) \times \nabla' \frac{1}{\mid \mathbf{r} - \mathbf{r}' \mid} d^{3}r', \\ \mathbf{B}^{R}\left(\mathbf{r}\right) &= -\frac{\mu_{0}}{4\pi} \sum_{i} \sigma_{i} \int_{V_{i}} \nabla' V\left(\mathbf{r}'\right) \times \nabla' \frac{1}{\mid \mathbf{r} - \mathbf{r}' \mid} d^{3}r', \end{split}$$

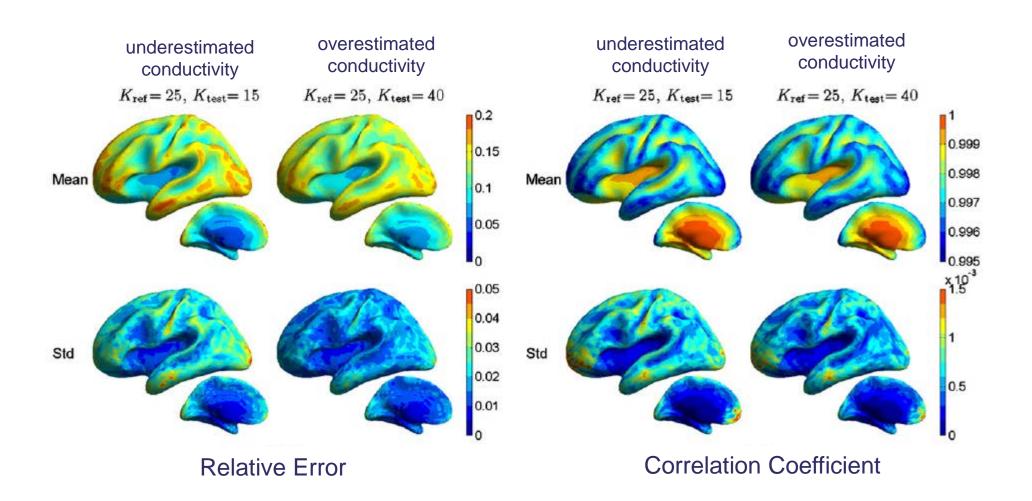
Heller & Volegov, in Magnetoencephalography by Supek & Aine (edts), Springer 2019

- Volume currents depend on conductivity distribution within the whole head volume.
- EEG measurements on the scalp are the result of volume currents, and are strongly affected by head geometry.
- MEG measurements are the sum of magnetic fields from primary and volume currents, but the magnetic fields of currents close to the source are much stronger than at larger distances.
- ➤ Thus, MEG signals are less affected by head geometry (e.g. skull and scalp). We usually only use one compartment (inner skull) for MEG (unless in combination with EEG).

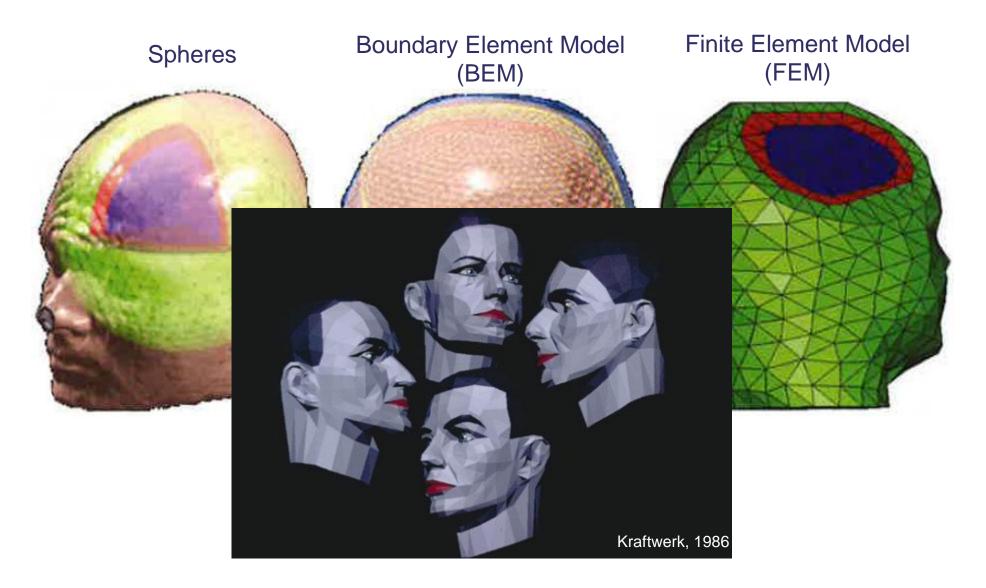
The Effect of Head Model Accuracy for MEG



Boundary Element Models Are Relatively Robust Against Conductivity Errors



Head Models With Different Levels of Detail



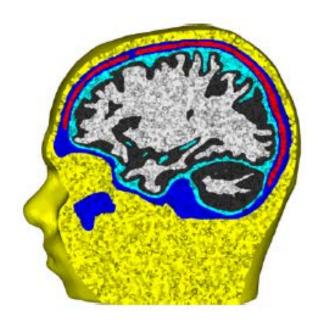
Finite Element Models (FEMs)

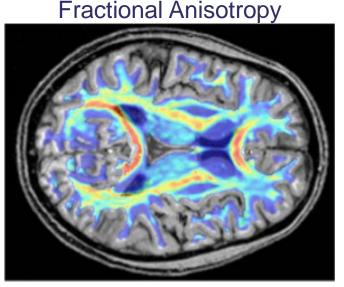
The use of 3-layer (brain, skull, scalp) BEM models based on individual MRI images is state-of-the-art for EEG/MEG source estimation.

For MEG-only, single shell BEMs and local/corrected sphere models can provide reasonable approximations.

But heads are more complex:

White Matter
Gray Matter
CSF
Skull
Compacta
Skull
Spongiosa
Skin





Vorwerk et al., NI 2014

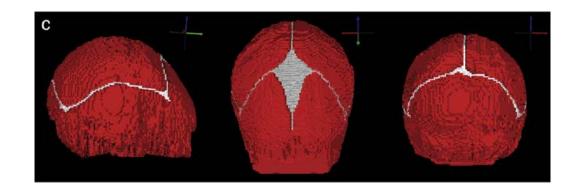
It is not obvious how to translate this into more accurate estimate for conductivity distributions.

Conductivities Of Tissues Can Only Be Approximated

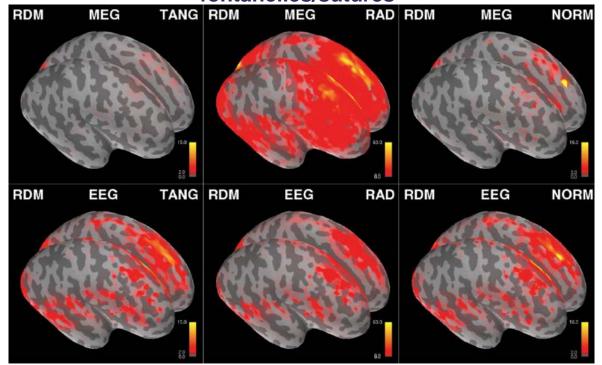
Table 2 Isotropic conductivity values of single tissue types used in human head volume conductor modeling

Tissue	Conductivity in S/m	Reference
Brain gray matter	0.45	Logothetis et al. 2007
Brain white matter	0.1	Akhtari et al. 2010
Spinal cord and cerebellum	0.16	Haueisen et al. 1995
Cerebrospinal fluid	1.79	Baumann et al. 1997
Hard bone (compact bone)	0.004	Tang et al. 2008
Soft bone (spongiform		
bone)	0.02	Akhtari et al. 2002
Blood	0.6	Gabriel et al. 2009
Muscle	0.1	Gabriel et al. 1996, 2009
Fat	0.08	Gabriel et al. 2009
Eye	1.6	Pauly and Schwan 1964; Lindenblatt and Silny 2001
Scalp	0.43	Geddes and Baker 1967
Soft tissue	0.17	Haueisen et al. 1995
Internal air	0.0001	Haueisen et al. 1995

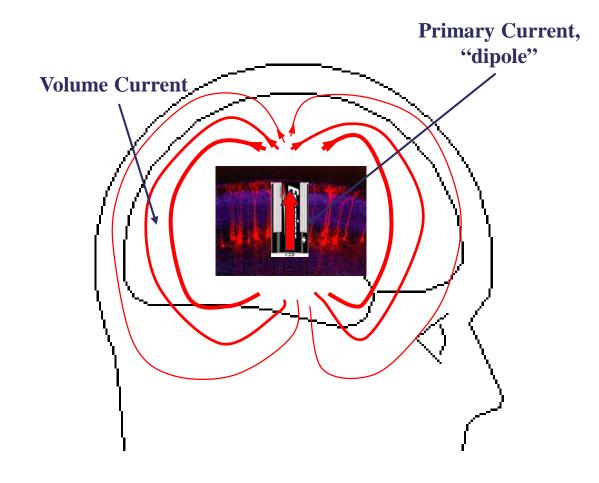
Infant Skulls – Fontanelles and Sutures

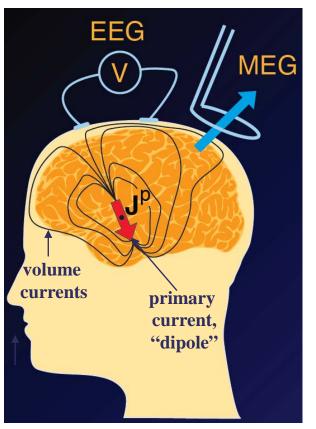


Relative error between models with and without fontanelles/sutures



Different Sensitivities of EEG and MEG





http://www.nmr.mgh.harvard.edu/meg/pdfs/talks/

All effects are instantaneous.

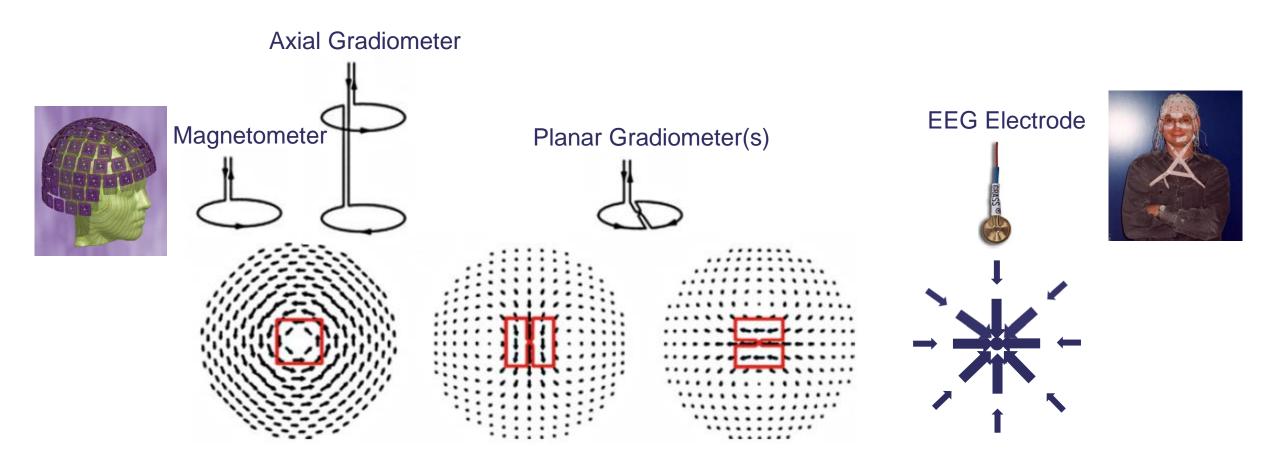
Volume currents affect both EEG and MEG –

but EEG more than MEG

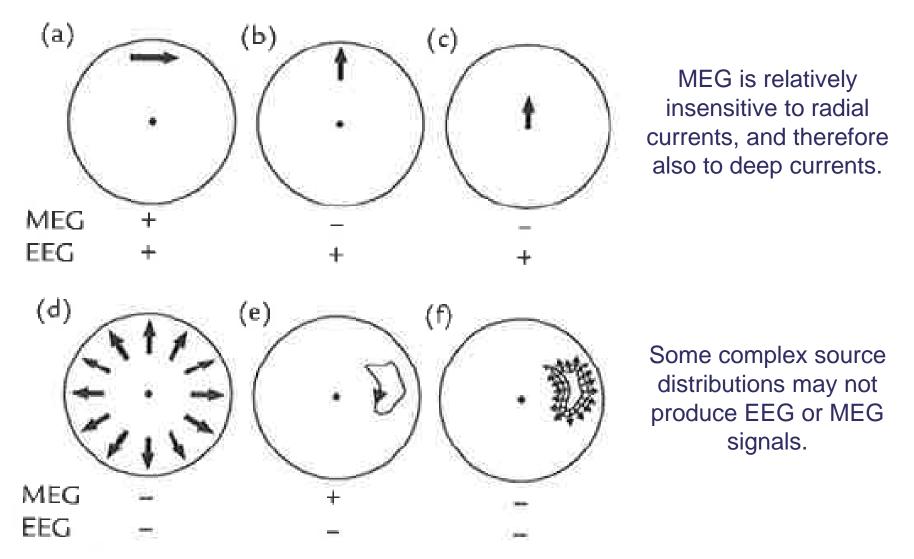
Different Sensors and their Sensitivities (Leadfields)

Leadfields are "sensitivity profiles" of individual sensors.

Each sensor is maximally sensitive to sources oriented along the arrows, and insensitive to sources perpendicular to the arrows.

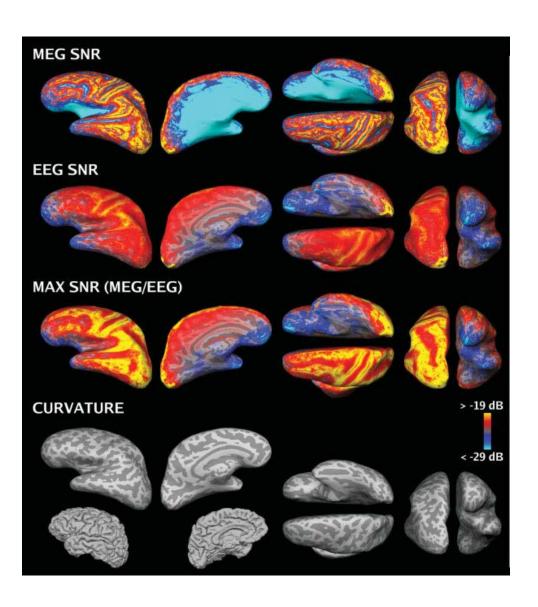


EEG and MEG Are Differentially Sensitive To Radial and Tangential Sources



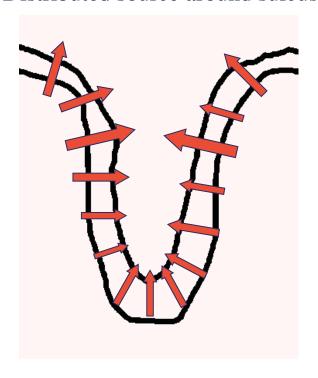
Sensitivity Maps

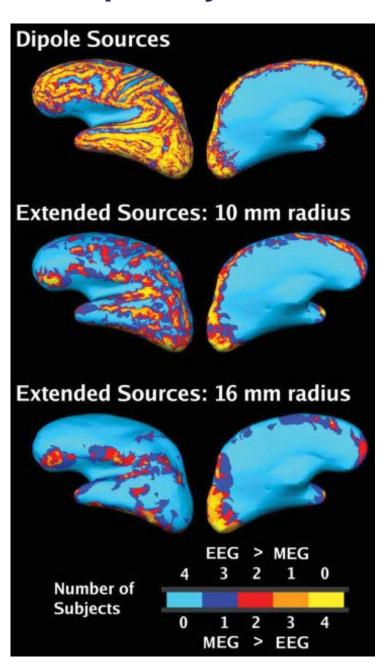
Sensor type, coverage and distance to sources strongly affect sensitivity and spatial resolution



MEG Is Less Sensitive To Spatially Extended Sources Than EEG

Distributed source around sulcus





Conclusion – Head Modelling

3-compartment BEM models are currently state-of-the-art for EEG/MEG source estimation.

Single-shell approximations are still common for MEG.

More detailed head models may increase accuracy, but require more accurate data and information, such as accurate MRI segmentations and conductivity values. (see e.g. Vorwerk et al., BioMeg Eng Online 2018) for Fieldtrip FEM pipeline)

There is no right or wrong, there are only different approximations – know your limits.

Fixing Head Models

https://mne.tools/stable/auto_tutorials/forward/80_fix_bem_in_blender.html





Thank you

