



MRC Cognition
and Brain
Sciences Unit



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EEG/MEG 3:

Functional Connectivity Analysis Cont'd

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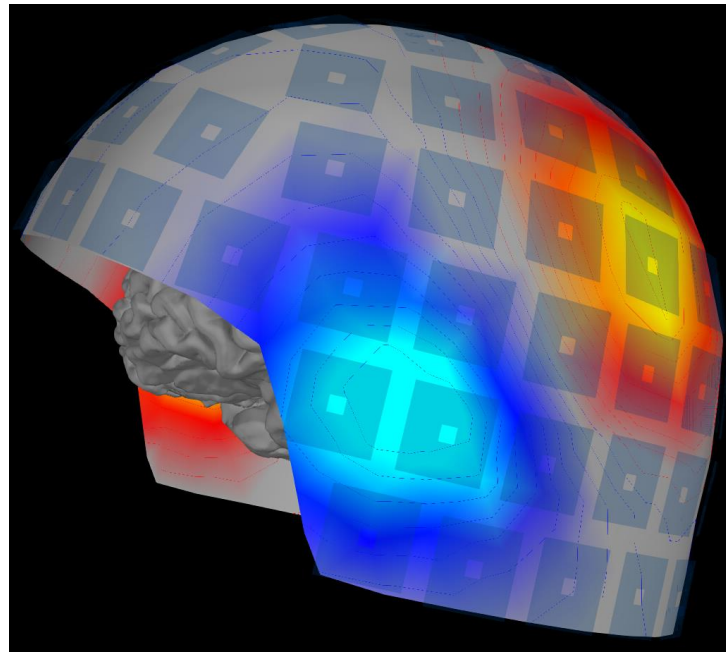
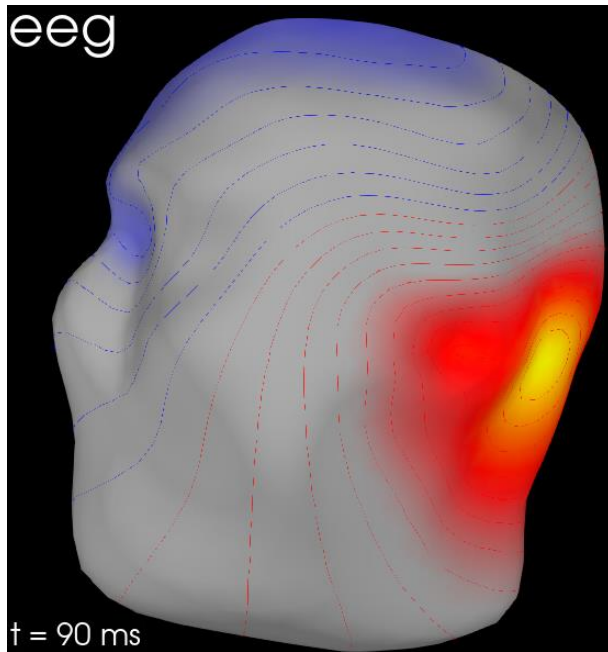
Functional Connectivity and Leakage

Olaf Hauk

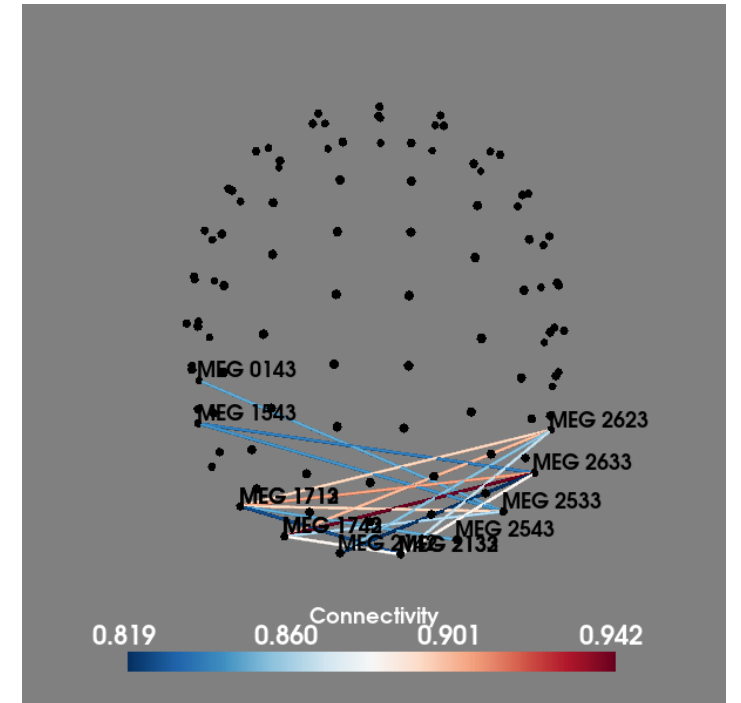
olaf.hauk@mrc-cbu.cam.ac.uk

“Connectivity” in sensor space is hard to interpret due to volume conduction

Tone to right ear

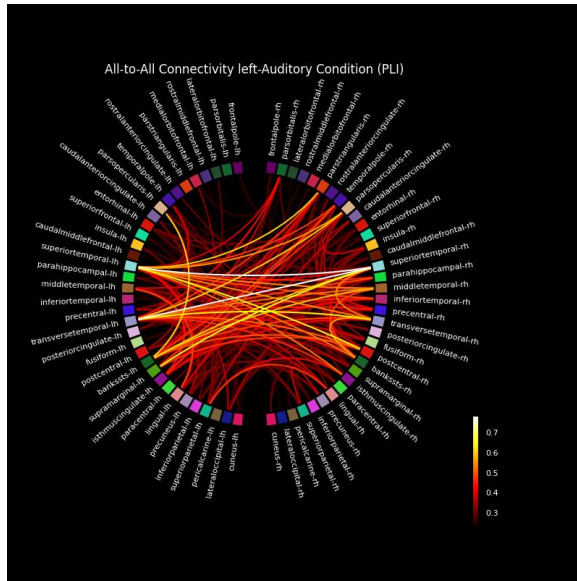


All-to-all “connectivity” for visual evoked response in sensor space

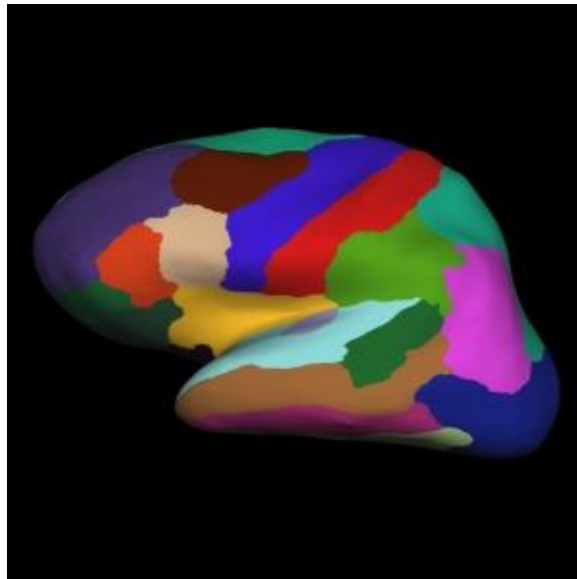


https://mne.tools/mne-connectivity/stable/auto_examples/sensor_connectivity.html

Connectivity in source space is limited by leakage

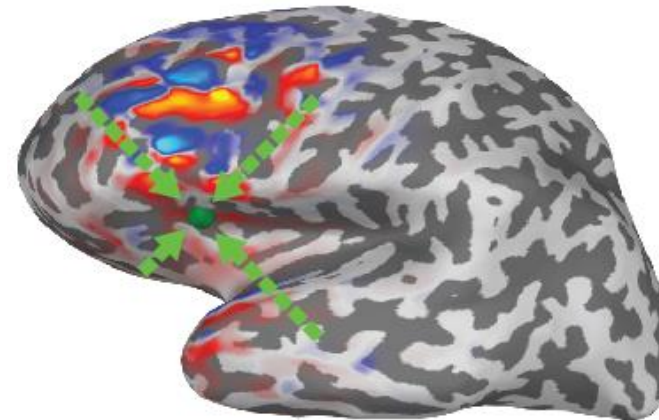


https://mne.tools/mne-connectivity/stable/auto_examples/mne_inverse_label_connectivity.html



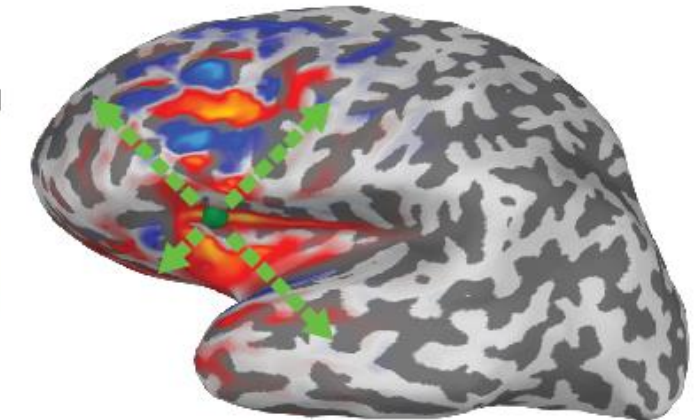
<https://surfer.nmr.mgh.harvard.edu/fswiki/CorticalParcellation>

Cross-Talk Function CTF



How other sources may affect the estimate for this source

Point-Spread Function PSF

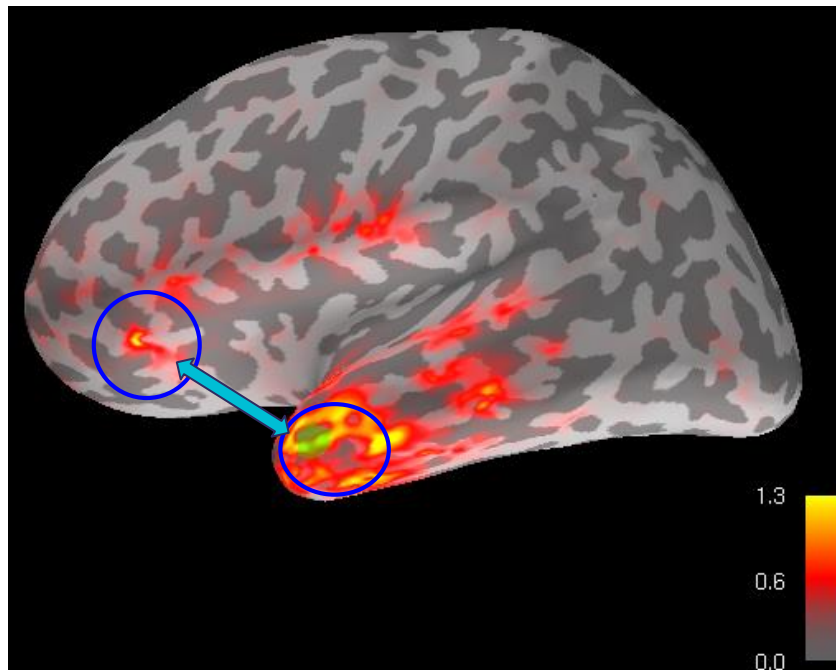


How this source affects estimates for other sources

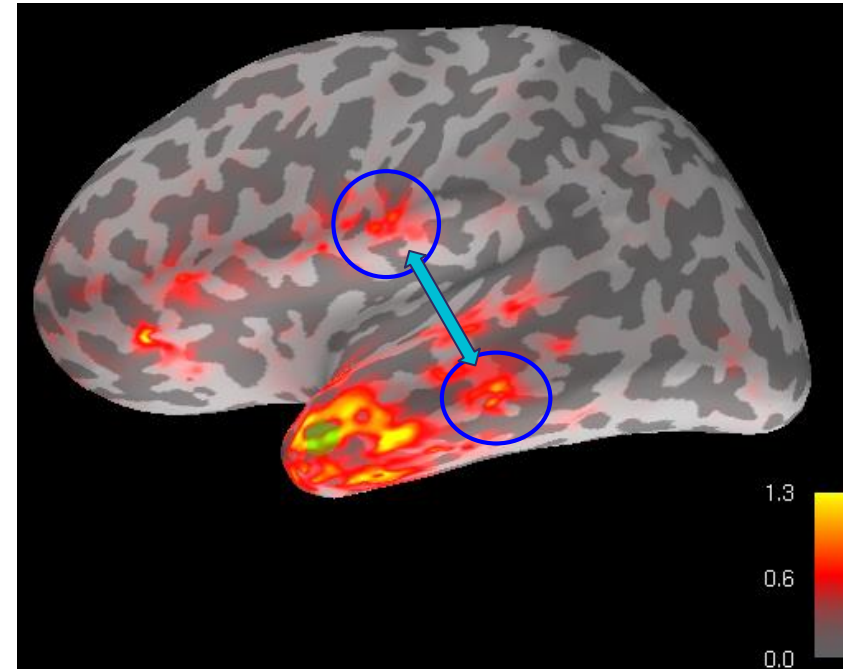
e.g. Hauk, Stenroos, Treder, Neuroimage 2022, <https://www.sciencedirect.com/science/article/pii/S1053811922002993>

The effect of leakage on (zero-lag) connectivity

Connectivity between two regions may reflect cross-talk from one of the regions



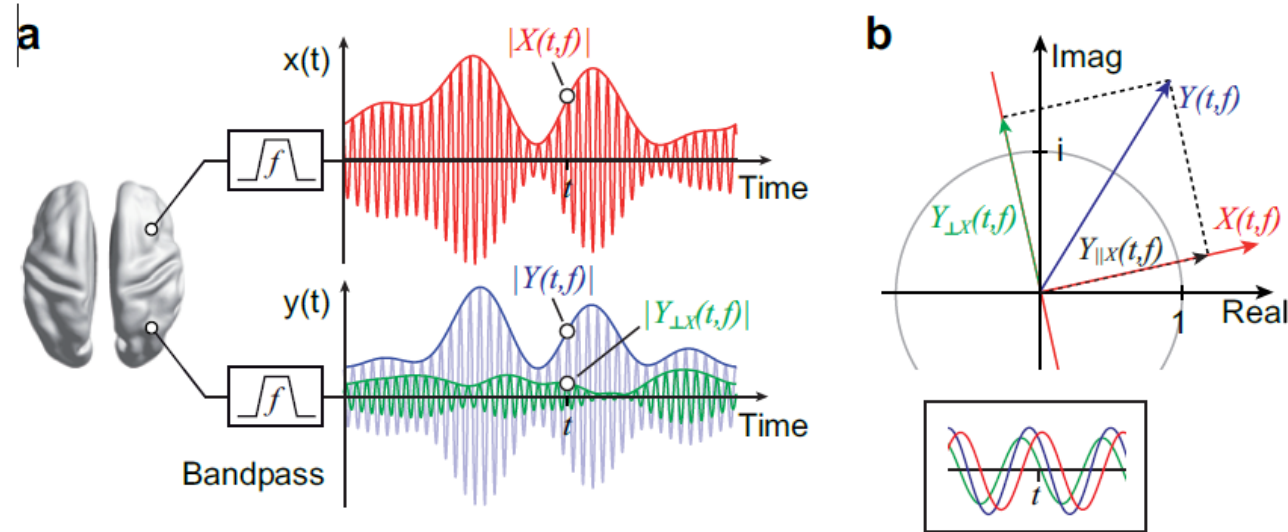
Connectivity between two regions may reflect cross-talk from a third region



One Possibility: Remove Zero-Lag Connectivity

Orthogonalisation of time courses, Partial regression

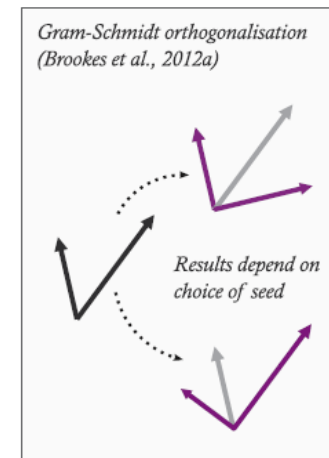
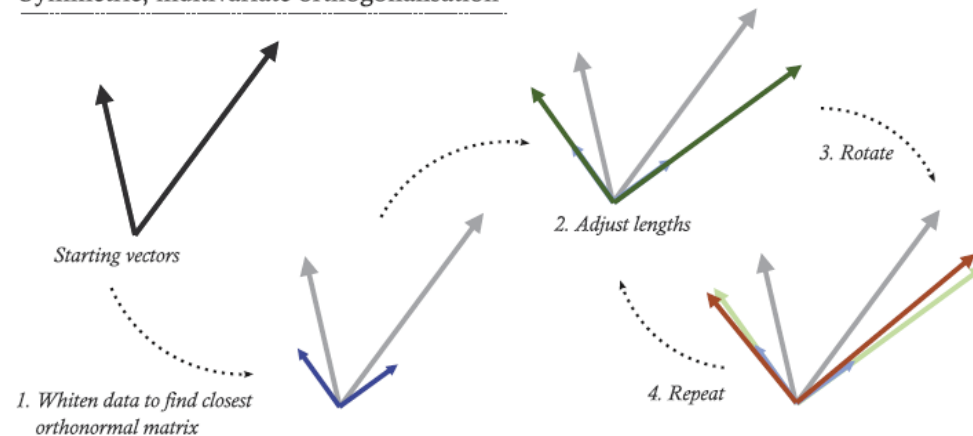
Bivariate:



Hipp et al., Nat Nsc 2012, <https://www.nature.com/articles/nn.3101>

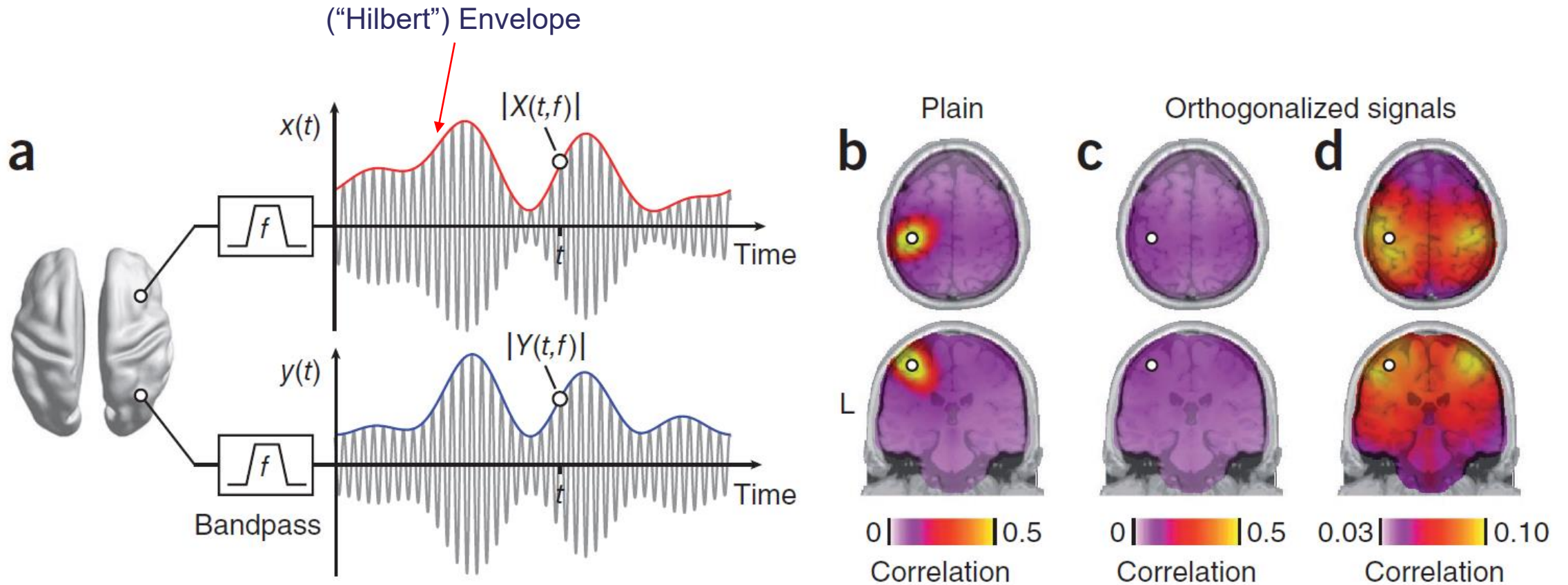
Multivariate:

Symmetric, multivariate orthogonalisation

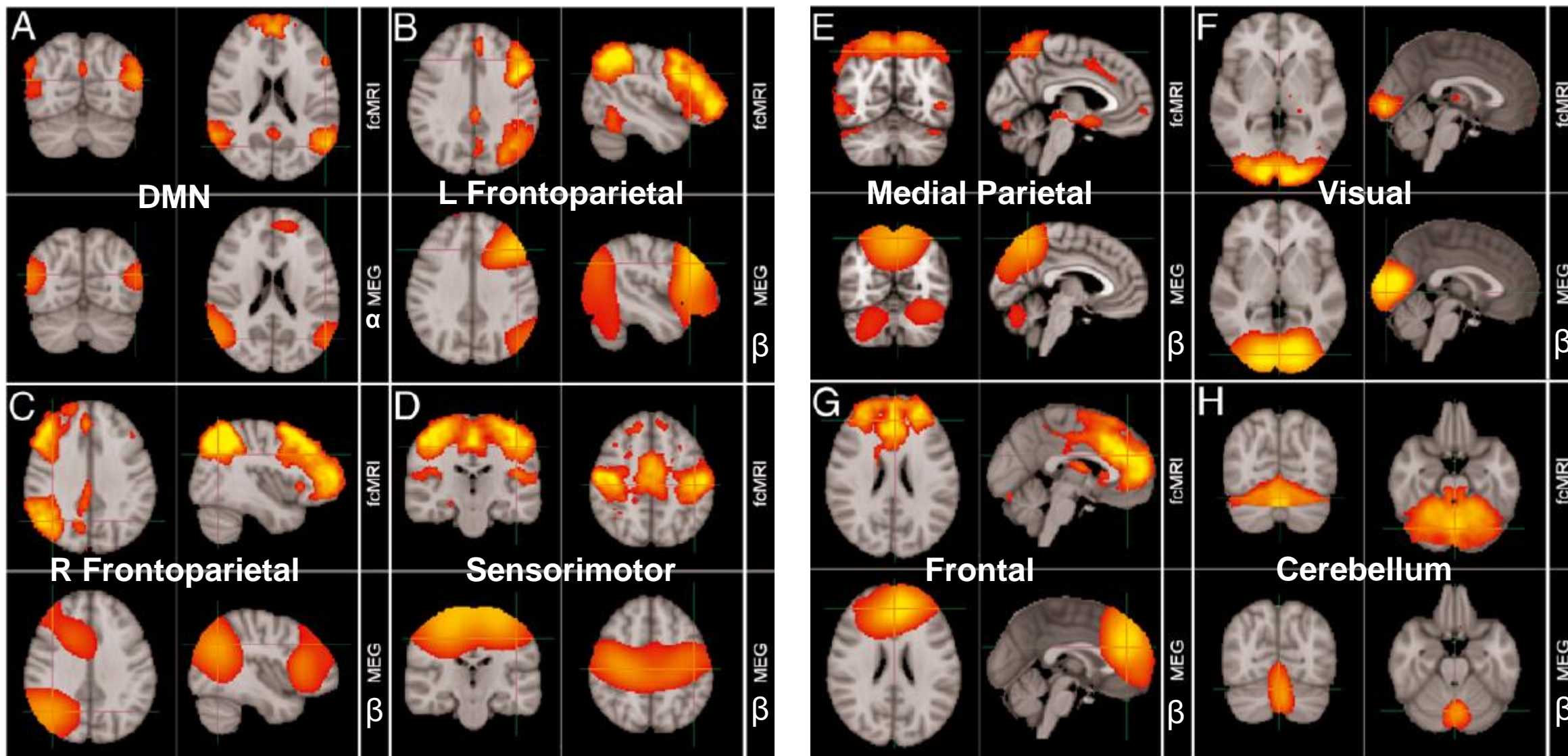


Colclough et al., NI 2015, <https://www.ncbi.nlm.nih.gov/pmc/articles/PMC4528074/>

Functional Connectivity of Resting State Activity



Functional Connectivity of Resting State Activity



Another Possibility: Ignore “Zero-Lag” Connectivity

E.g.: Imaginary Part of Coherency

In spectral connectivity measures like Coherence, only use the imaginary part of the signal, which is unaffected by zero-lag connectivity (phase differences of zero are only represented in the real part).

Nolte et al., Clin Neurophysiol 2004, <https://www.sciencedirect.com/science/article/pii/S1388245704001993>

Ewald et al., NI 2012, <https://pubmed.ncbi.nlm.nih.gov/22178298/>

Pascual-Marqui, arXiv 2007a and 2007b, <https://arxiv.org/abs/0706.1776>, <https://arxiv.org/abs/0711.1455>

Note: “Non-zero-lag methods” may also ignore true zero-lag connectivity, e.g. for bilateral sources – one may throw out the child with the bath water.

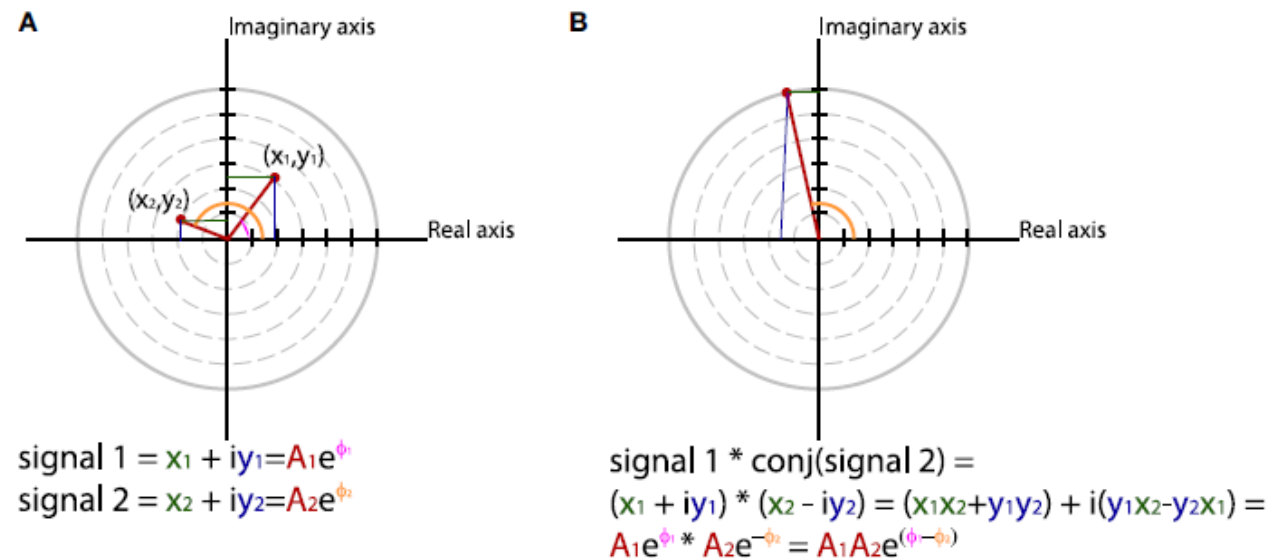
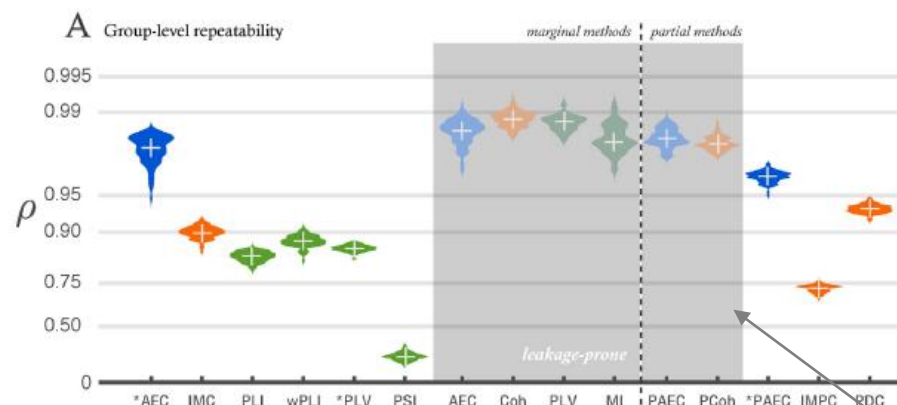


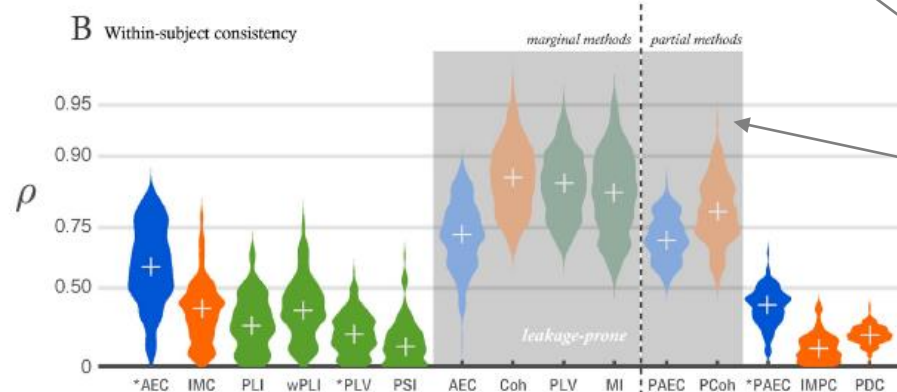
FIGURE 2 | Using polar coordinates and complex numbers to represent signals in the frequency domain. **(A)** The phase and amplitude of two signals. **(B)** The cross-spectrum between signal 1 and 2, which corresponds to multiplying the amplitudes of the two signals and subtracting their phases.

Leakage and Reliability of Functional Connectivity Methods

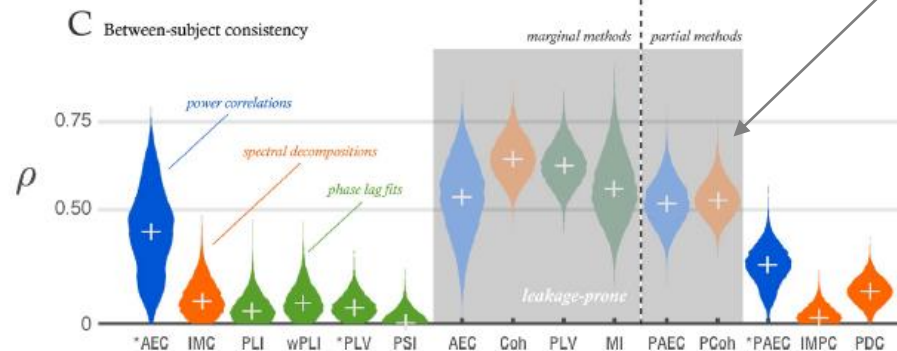
Group-level repeatability



Within-subject consistency



Between-subject consistency



leakage-prone

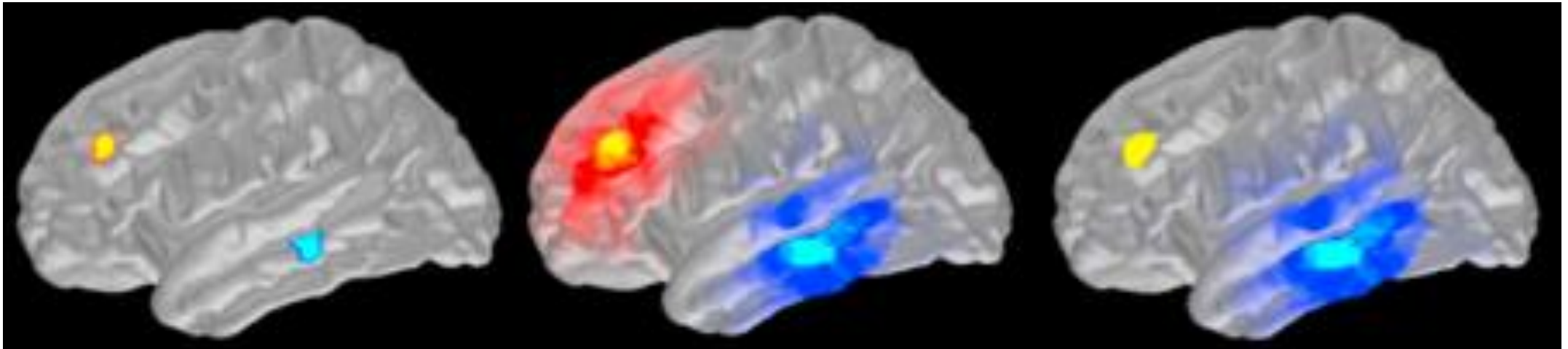
Removing zero-lag effects does not remove leakage altogether

The inverse problem still exists

True non-zero-lag
connectivity

Zero-lag measures

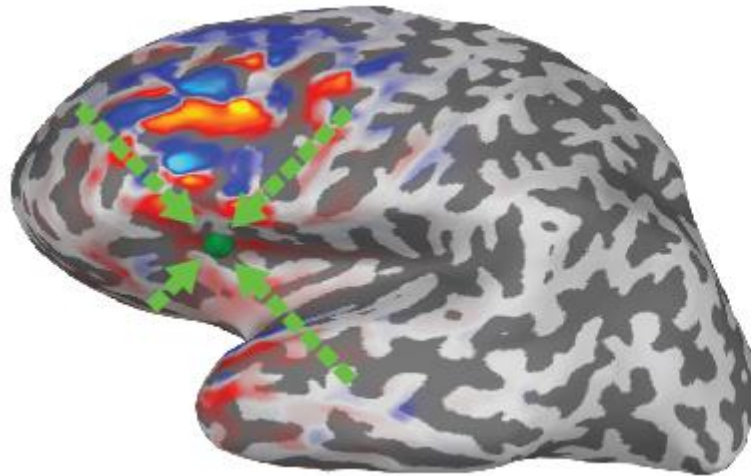
Non-zero-lag
measures



Spatial Resolution / Leakage:

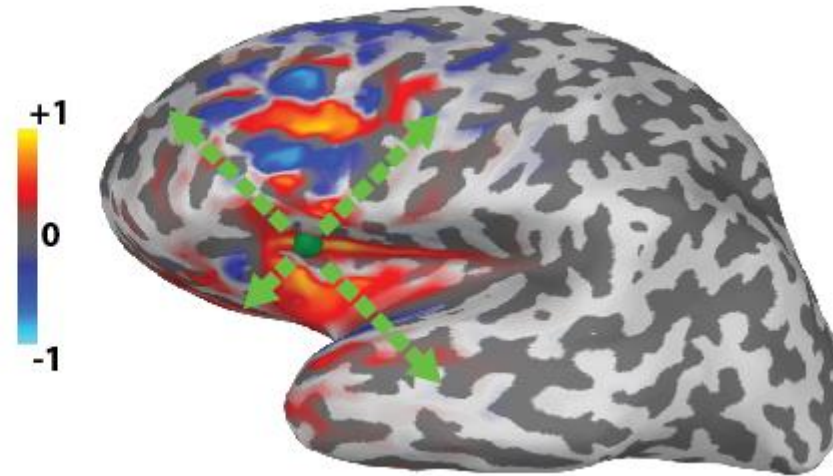
Point-Spread and Cross-Talk

Cross-Talk Function
(CTF)



How other sources may affect the estimate for this source

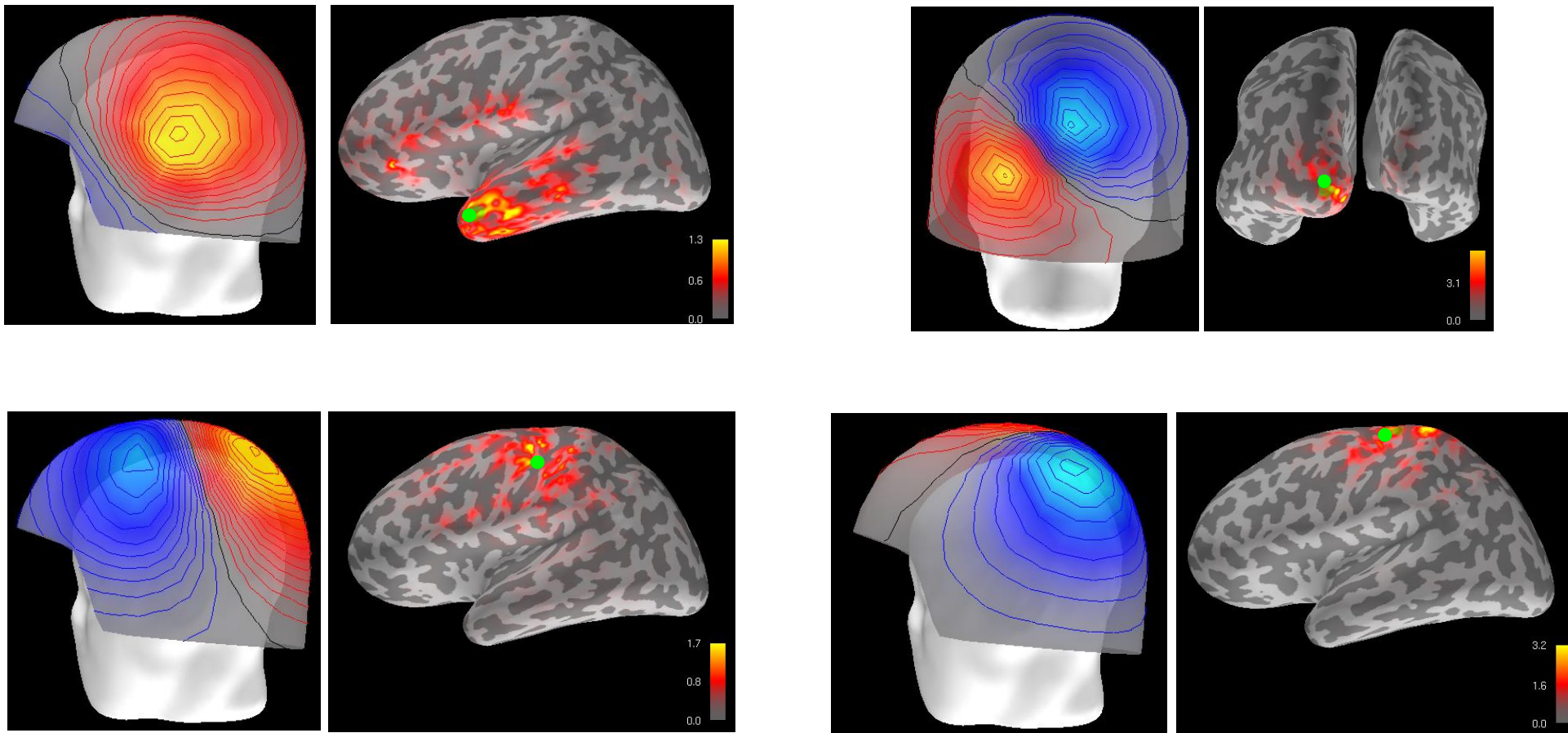
Point-Spread Function
(PSF)



How this source affects estimates for other sources

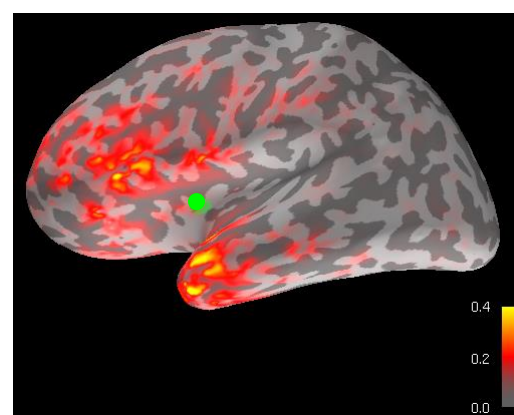
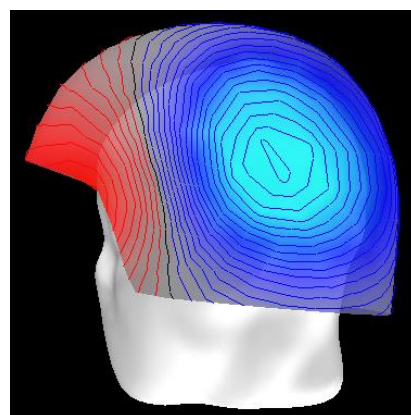
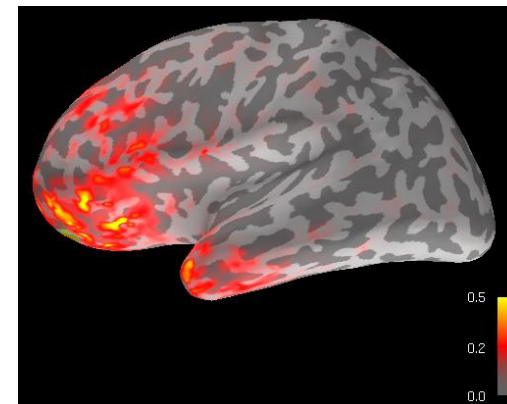
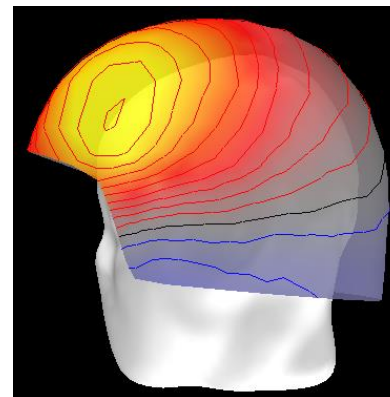
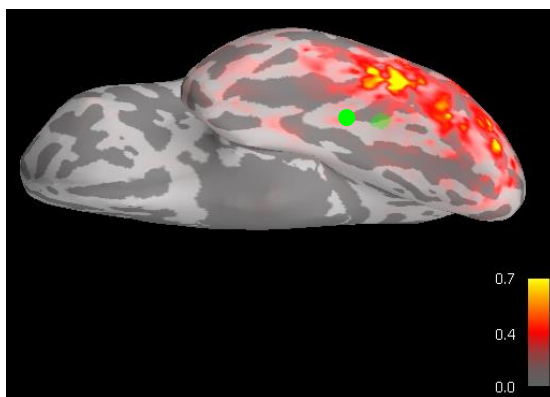
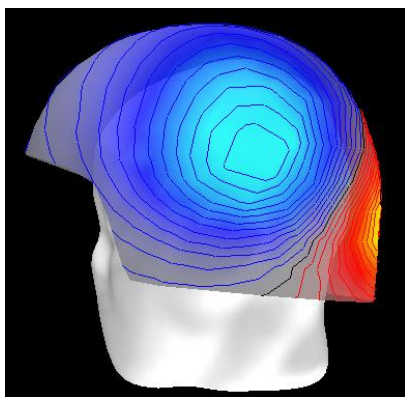
PSFs and CTFs for Some ROIs

For MNE, PSFs and CTFs turn out to be the same



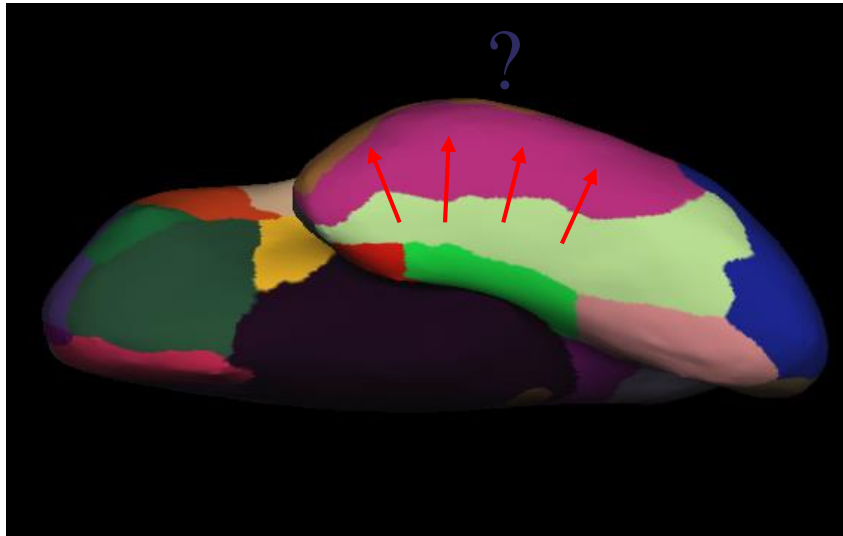
PSFs and CTFs for Some ROIs

For MNE, PSFs and CTFs turn out to be the same

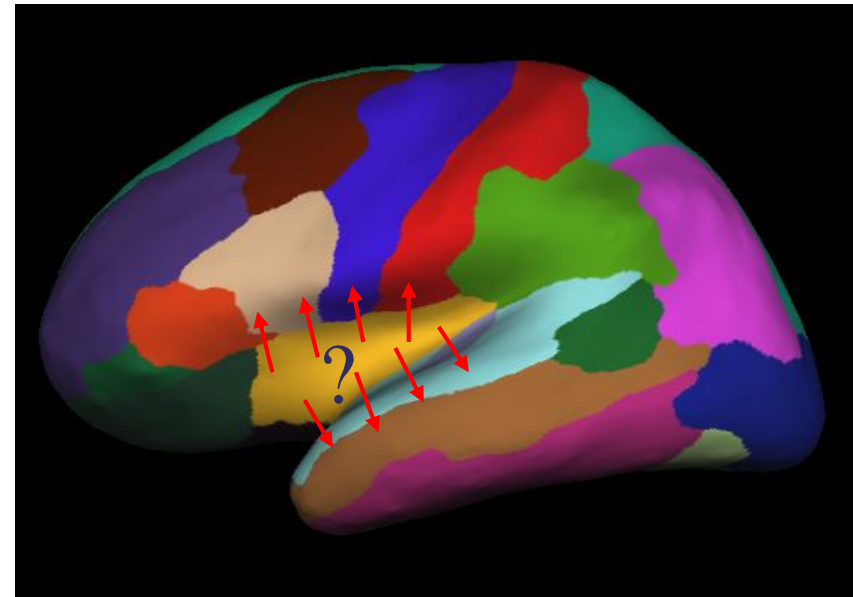


Localisation Bias Has Consequences for ROI analysis

PSFs/CTFs Can Tell You How It Looks Like

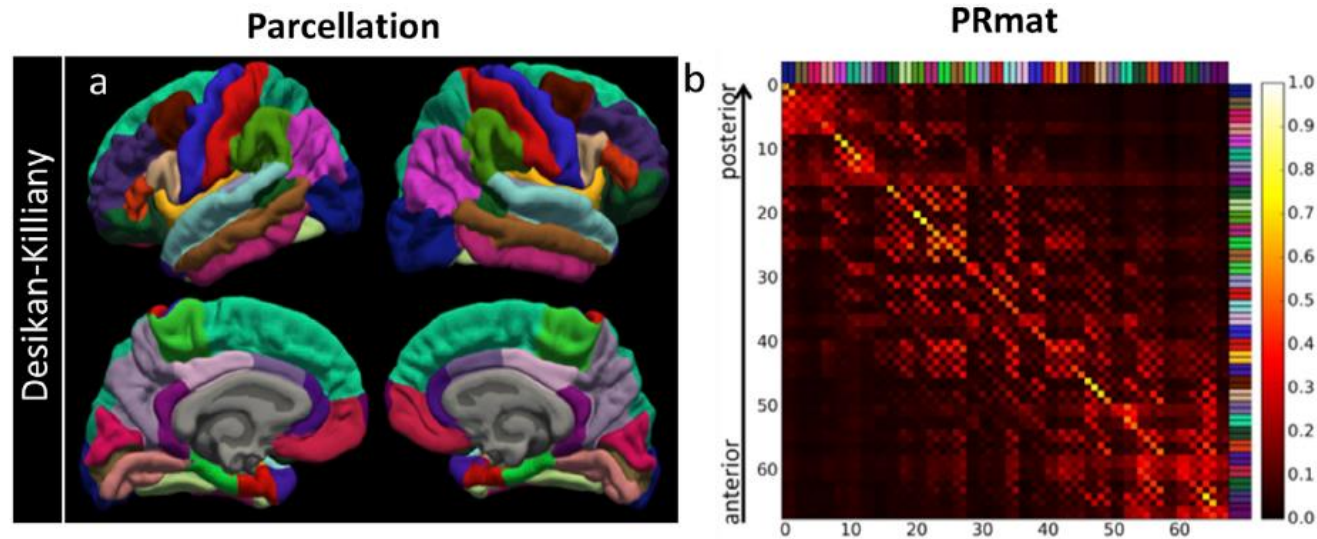


Desikan-Killiany Atlas parcellation

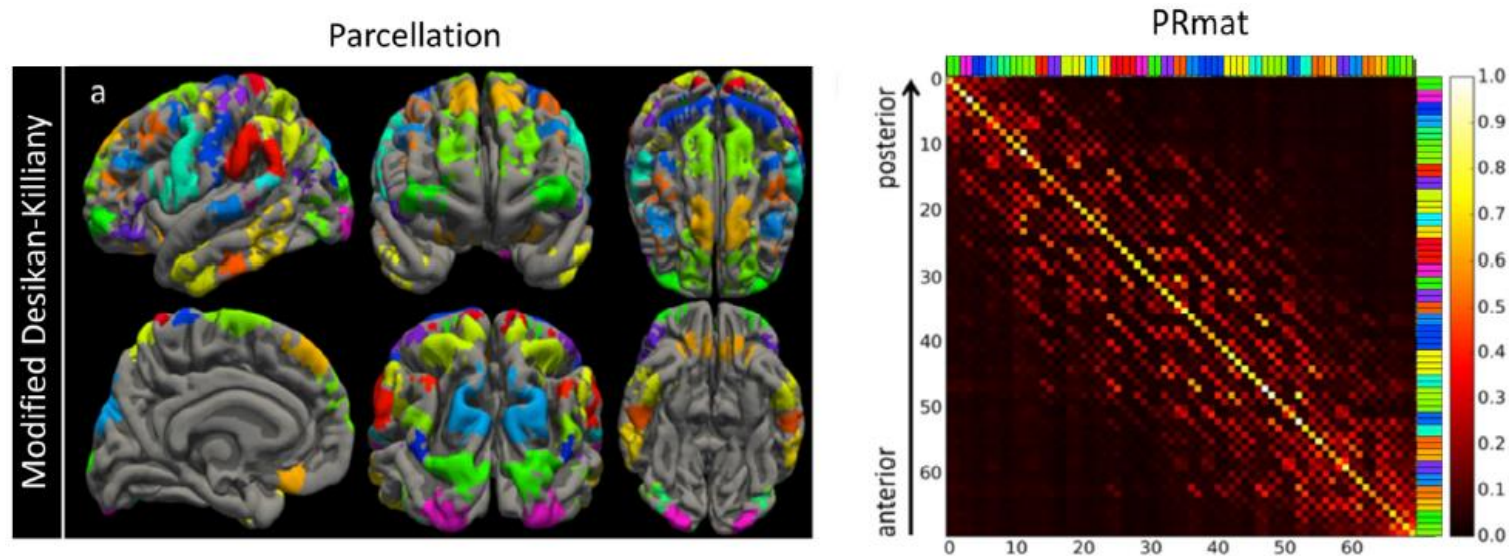


Adaptive cortical parcellation based on resolution matrix

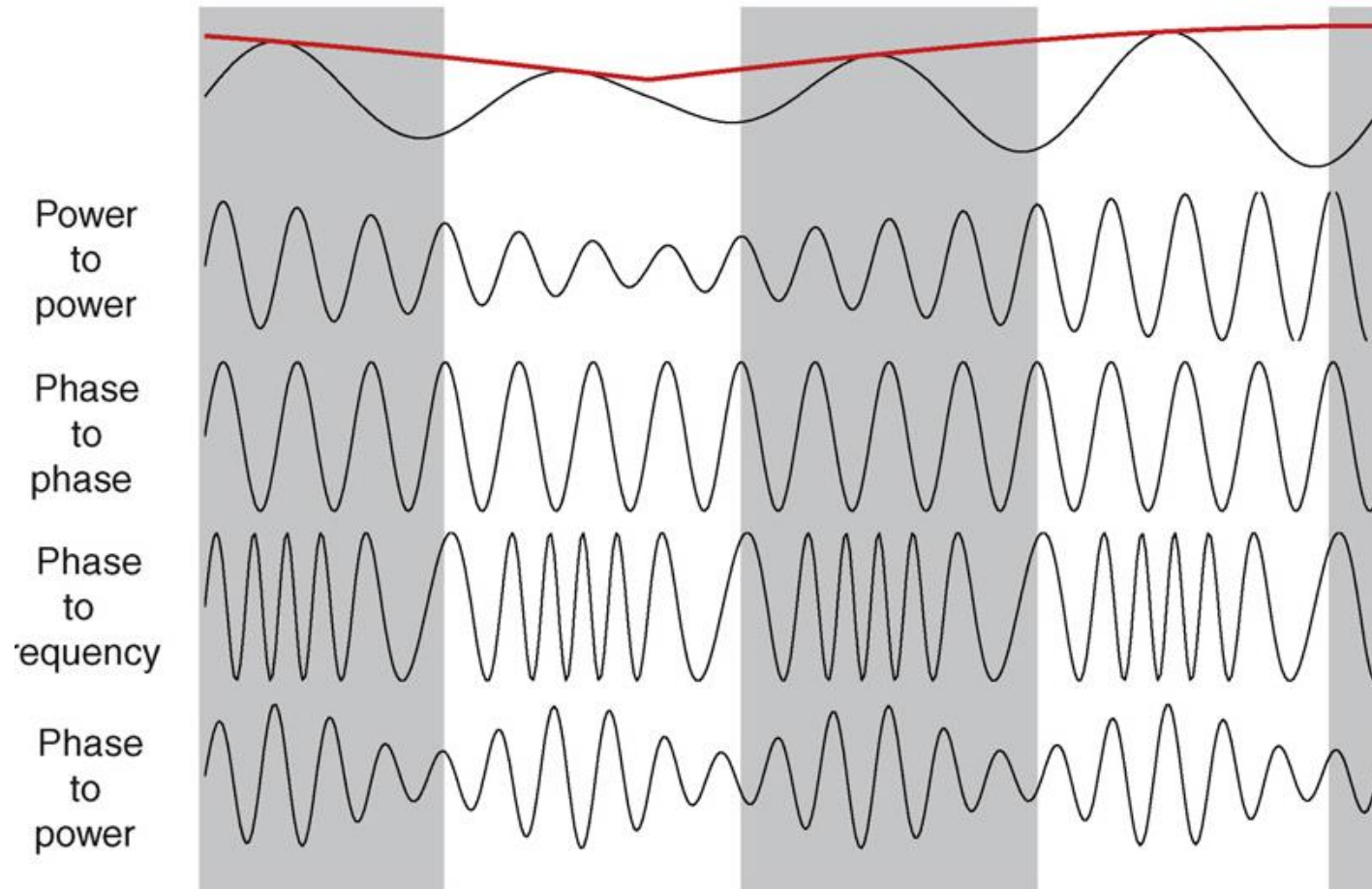
Original Parcellation



Modified Parcellation

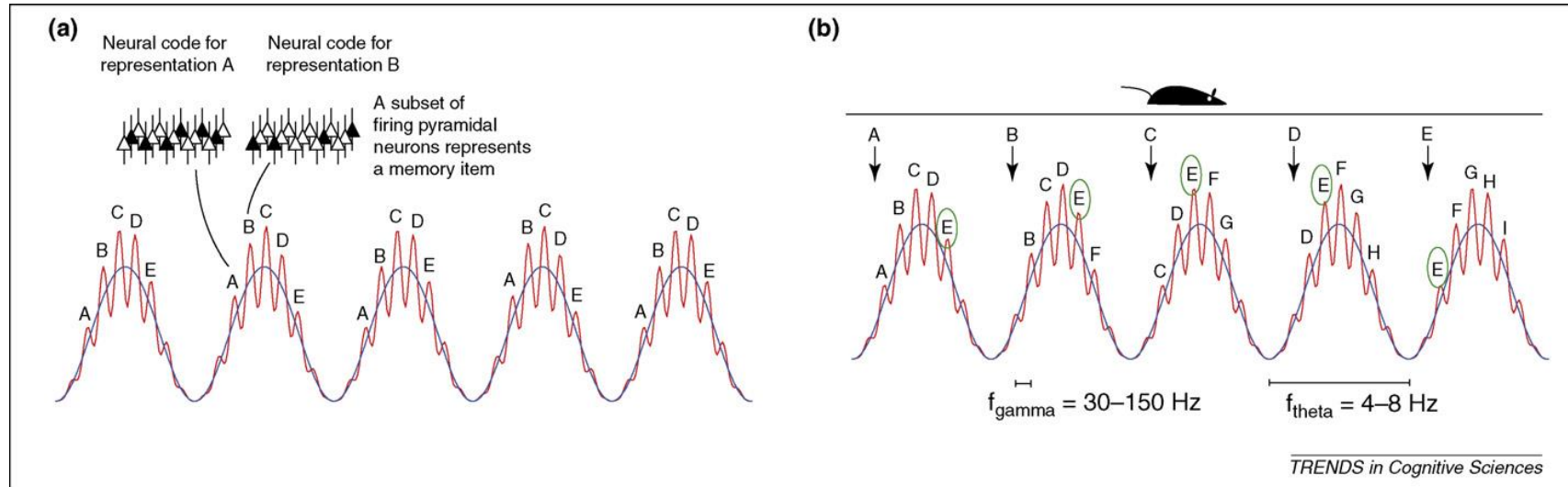


Cross-Frequency Coupling



Jensen & Colgin, TICS 2007

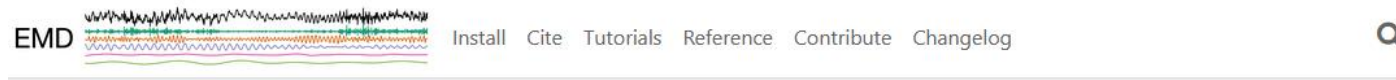
For Example: Theta-Gamma Coupling



Jensen & Colgin, TICS 2007

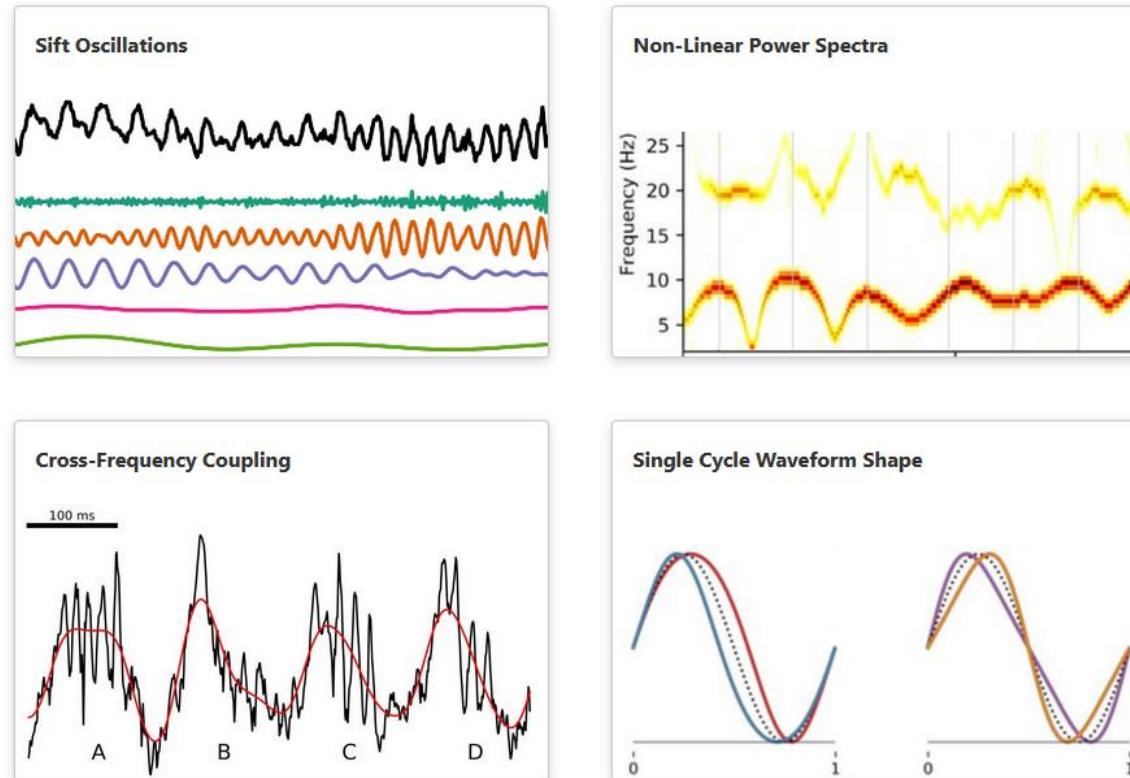
Figure 2. Models proposing computational roles for cross-frequency interactions between theta and gamma oscillations by means of phase coding. (a) In a model for working memory, individual memory representations are activated repeatedly in every theta cycle [10] (reviewed in Ref. [11]). Each memory representation is represented by a subset of neurons in the network firing synchronously. Because different representations are activated in different gamma cycles, the gamma rhythm serves to keep the individual memories segmented in time. The number of gamma cycles per theta cycle determines the span of the working memory. (b) A model accounting for theta phase precession in rats. As a rat advances through an environment, positional information is passed to the hippocampus. This activates the respective place cell representations, which provokes the prospective recall of upcoming positions. In each theta cycle, time-compressed sequences are recalled: one representation per gamma cycle. Consider the firing of a cell participating in representation E. As the rat advances, this cell fires earlier in the theta cycle, thus accounting for phase precession. According to this scheme, the number of gamma cycles per theta cycle is related quantitatively to the phase precession [13].

Python Toolbox for Cross-Frequency Coupling and more



Empirical Mode Decomposition in Python

Python tools for the extraction and analysis of non-linear and non-stationary oscillatory signals.



<https://emd.readthedocs.io/en/stable/index.html>

More Python Toolboxes:

bycycle - cycle-by-cycle analysis of neural oscillations

repo status **Active** pypi **v1.1.0** build **passing** codecov **95%** license Apache License, 2.0 python **3.6 | 3.7 | 3.8 | 3.9 | 3.10 | 3.11** publication **10.1152/jn.00273.2019**

ByCycle is a module for analyzing neural oscillations in a cycle-by-cycle approach.

Overview

bycycle is a tool for quantifying features of neural oscillations in the time domain, as opposed to the frequency domain, using a cycle-by-cycle approach. Rather than applying narrowband filters and other methods that use a sinusoidal basis, this approach segments a recording into individual cycles and directly measures each of their properties including amplitude, period, and symmetry.

This is most advantageous for analyzing the waveform shape properties of neural oscillations. It may also provide advantages for studying traditional amplitude and frequency effects, as well. Using cycle properties can also be used for burst detection.

A full description of the method and approach is available in the paper below.

<https://bycycle-tools.github.io/bycycle/>

FOOOF - fitting oscillations & one over f

repo status **Active** pypi **v1.1.0** build **passing** codecov **98%** license Apache License, 2.0 python **3.6 | 3.7 | 3.8 | 3.9 | 3.10 | 3.11** paper **nn10.1038**

FOOOF is a fast, efficient, and physiologically-informed tool to parameterize neural power spectra.

Overview

The power spectrum model conceives of a model of the power spectrum as a combination of two distinct functional processes:

- An aperiodic component, reflecting $1/f$ like characteristics, with
- A variable number of periodic components (putative oscillations), as peaks rising above the aperiodic component

This model driven approach can be used to measure periodic and aperiodic properties of electrophysiological data, including EEG, MEG, ECoG and LFP data.

The benefit of fitting a model in order to measure putative oscillations, is that peaks in the power spectrum are characterized in terms of their specific center frequency, power and bandwidth without requiring predefining specific bands of interest and controlling for the aperiodic component. The model also returns a measure of this aperiodic components of the signal, allowing for measuring and comparison of $1/f$ -like components of the signal within and between subjects.

<https://fooof-tools.github.io/fooof/>

More connectivity...

Most of the previously introduced measures are spectral measures, i.e. they are computed for specific frequencies (or frequency bands).

They rely on the assumption that brain signals can meaningfully be decomposed into “oscillations” or “frequency bands”.

This is a big assumption, and may not be the case for all modalities, stimuli, tasks etc., or may not even be true in general.

Therefore...

Non-Spectral and Effective Connectivity

Granger Causality: Is one time series useful to predict another?

$x(t)$ Granger-causes $y(t)$ if past values of $x(t)$ add information to past values of $y(t)$ for predicting future values of $y(t)$.

http://www.scholarpedia.org/article/Granger_causality

Multivariate Granger Toolbox: <http://www.sussex.ac.uk/sackler/mvgc/>

<http://journal.frontiersin.org/article/10.3389/fnsys.2015.00175/full>

Structural Equation Modelling (SEM):

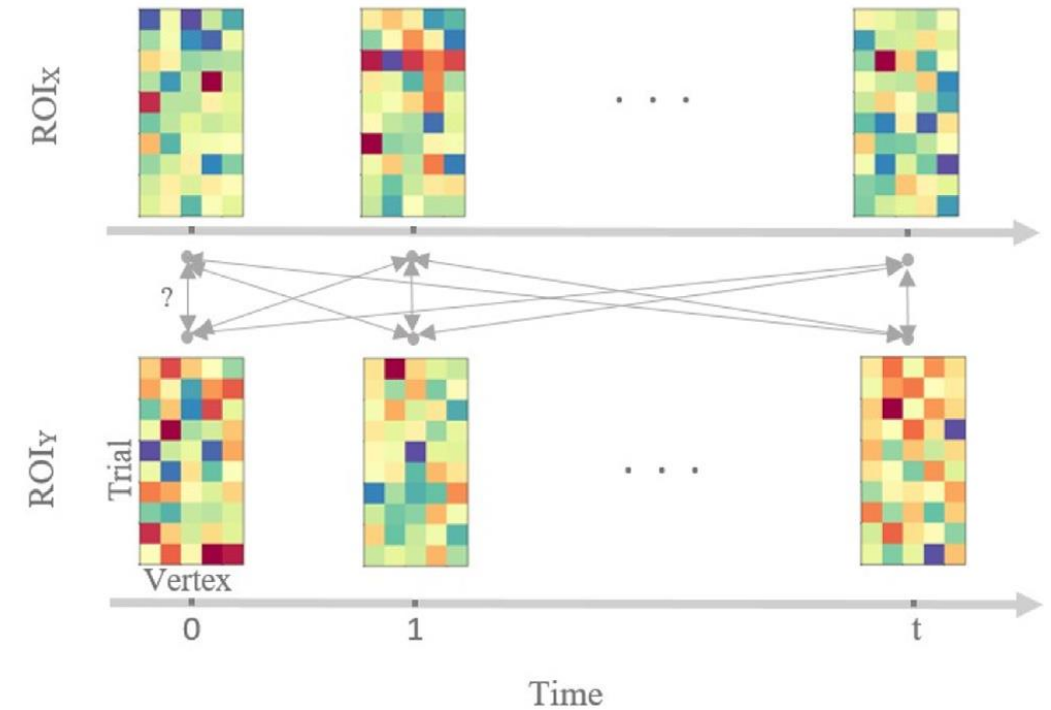
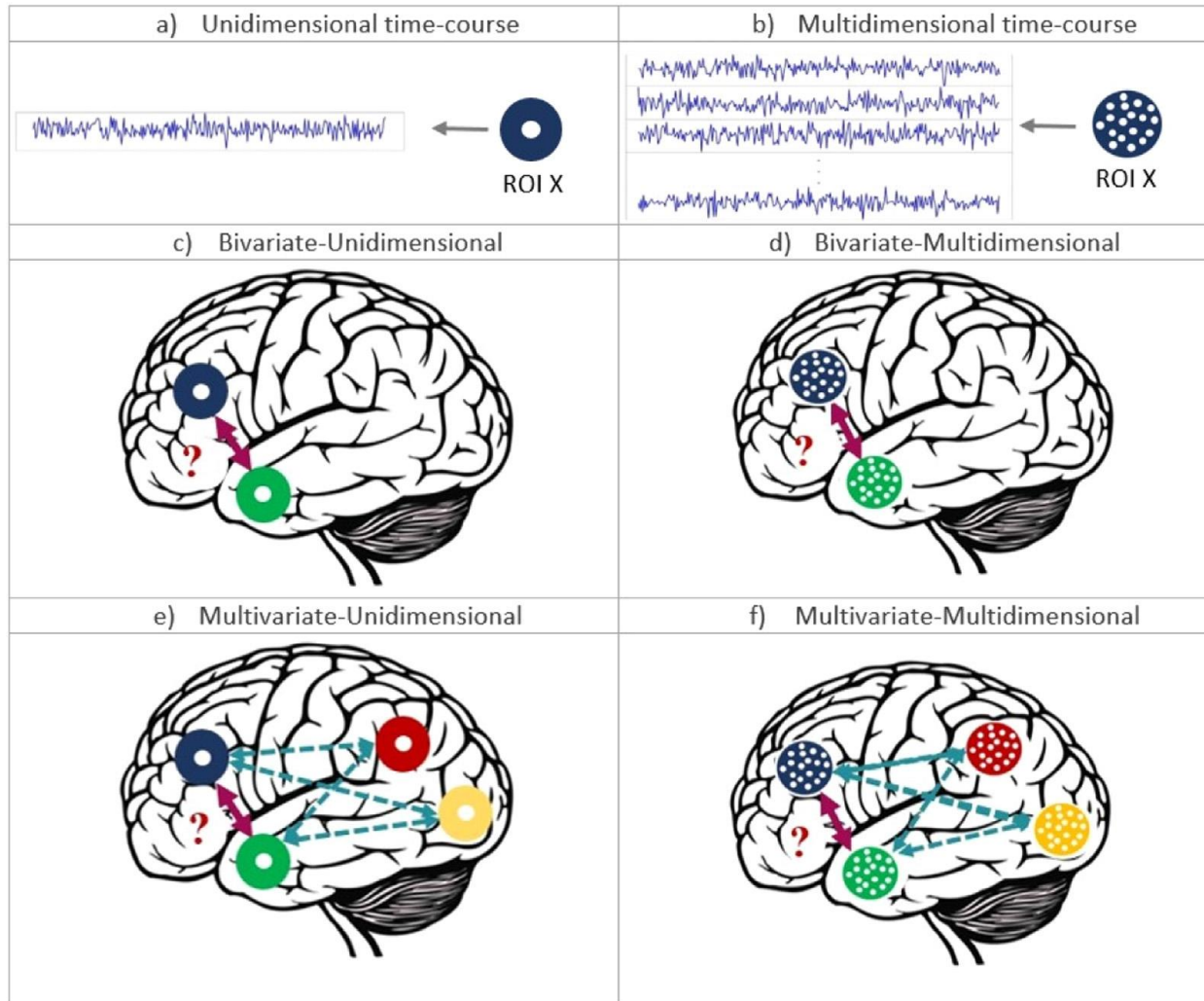
Models covariance structure of brain activation across brain regions (e.g. “path analysis”).

Dynamic Causal Modelling (DCM):

Models brain dynamics across regions as differential equations, in combination with Bayesian parameter/model estimation.

http://www.scholarpedia.org/article/Dynamic_causal_modeling

Multi-Variate and Multi-Dimensional Connectivity



Rahimi et al., NI 2022, <https://pubmed.ncbi.nlm.nih.gov/36813063/>

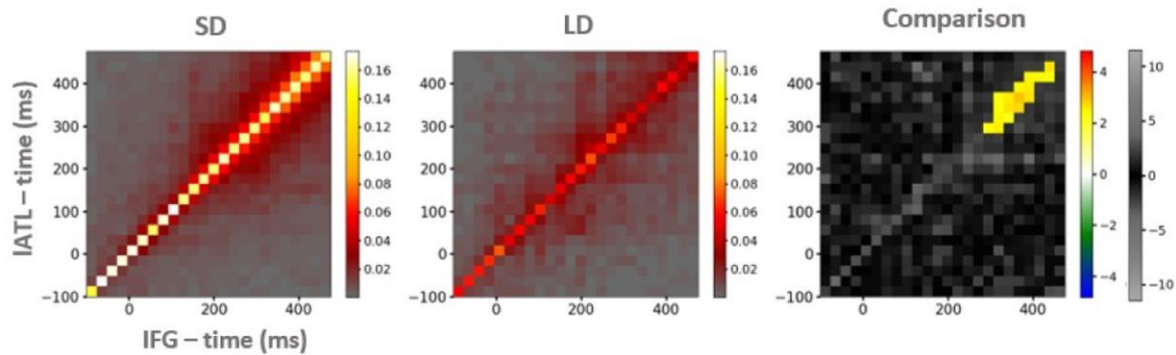
Also:

Basti/Nili et al., NI 2020, <https://www.sciencedirect.com/science/article/pii/S1053811920306650>, Anzellotti & Coutanche, T Cogn Sci 2018, <https://pubmed.ncbi.nlm.nih.gov/29305206/>,

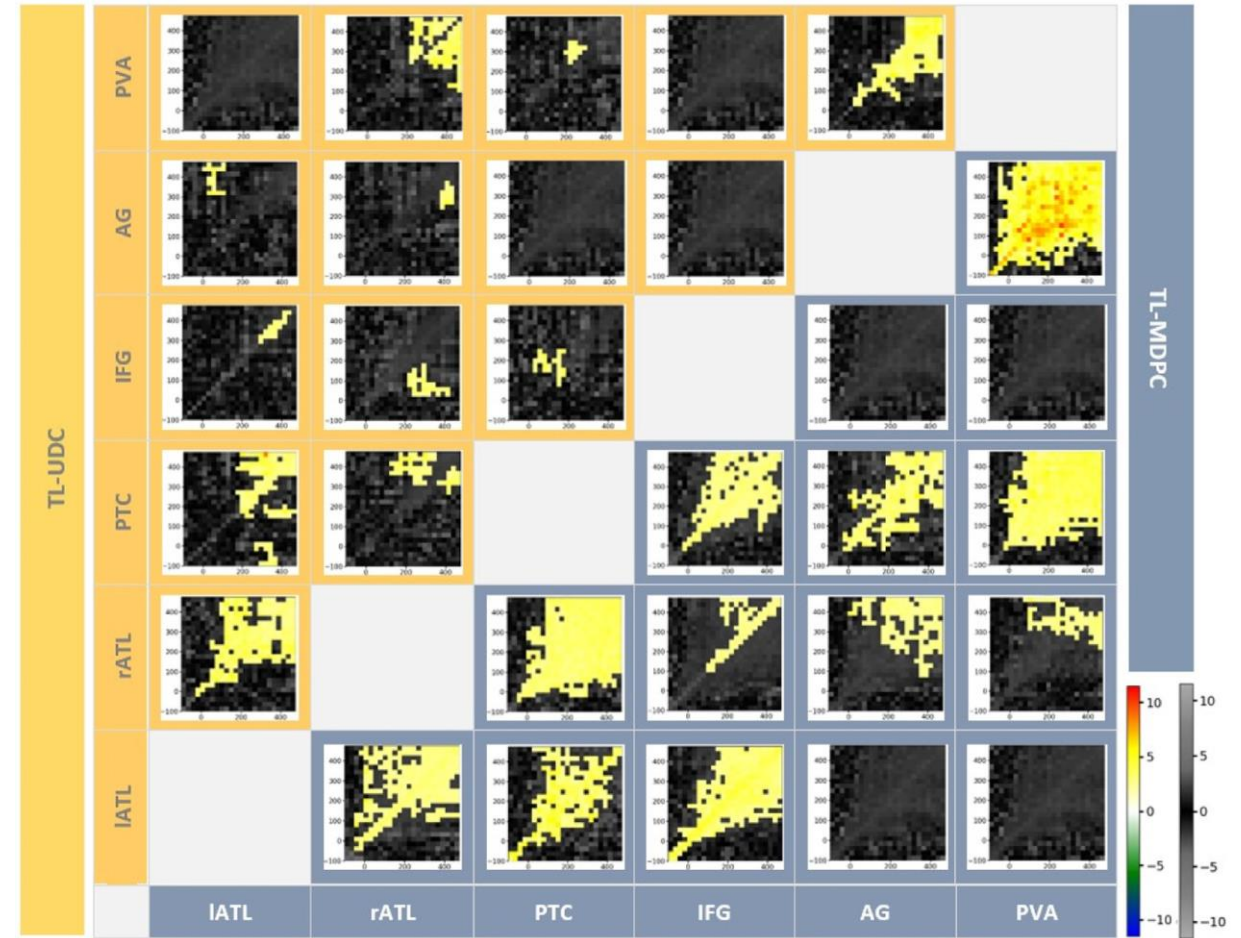
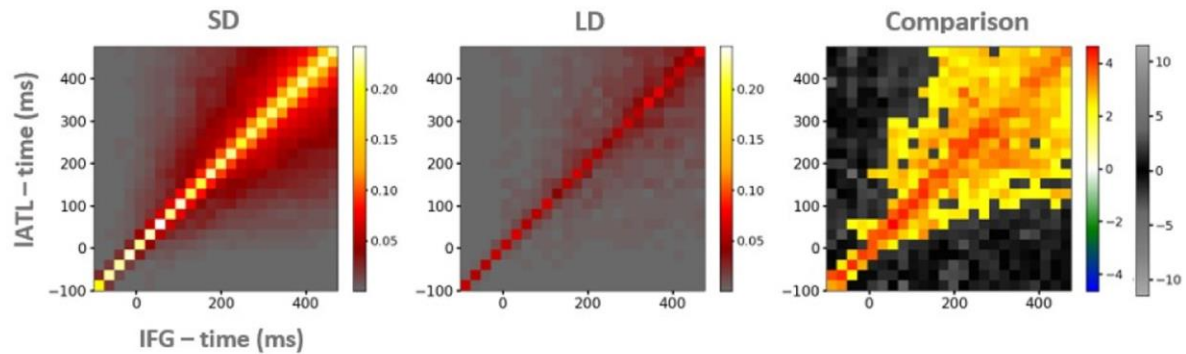
Basti et al., PLoS 2019, <https://journals.plos.org/plosone/article/comments?id=10.1371/journal.pone.0223660>

Multi-Dimensional Connectivity

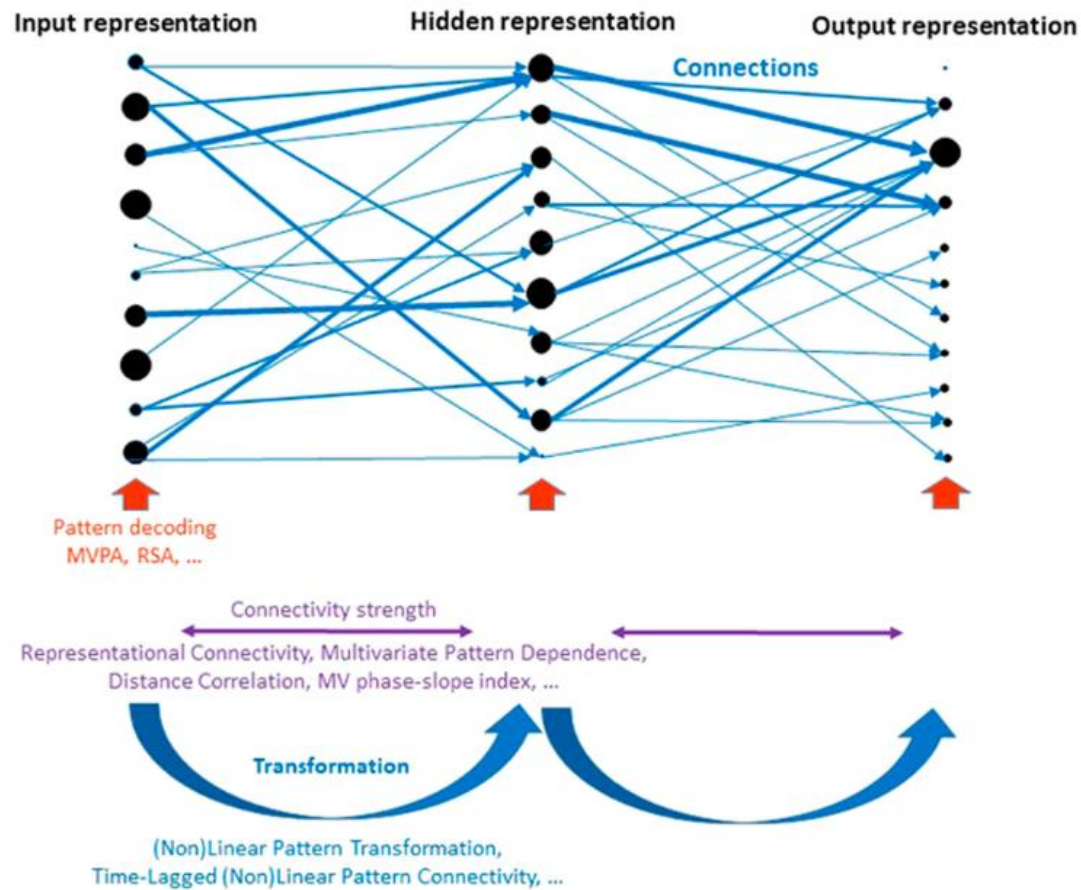
a) TL-UDC



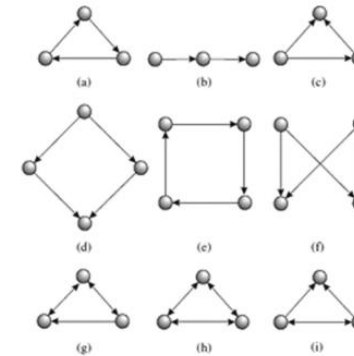
b) TL-MDPC



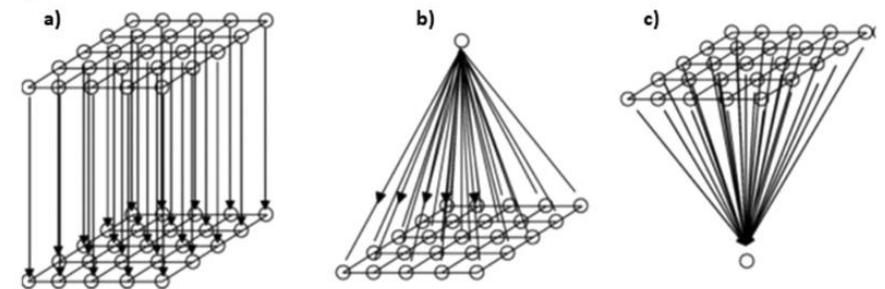
“Transforming” Neuroscience



A)



B)





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Thank you