

INTRODUCTION

Electromyography (EMG) is widely used for controlling functional prosthetics. However, EMG signals for the same movements change with variations in limb position and lowers the accuracy in control schemes [1]. Most previous studies have utilized classification for pattern recognition when changing limb position, with a negative effect in performance. Linear regression is a newer method in control of myoelectric prosthetics, which has proven to yield robust simultaneous and proportional control [2]. Only the RMS feature was previously tested in variations of limb positions in regression-based control [3]. This study investigated the effect of limb position in a linear regression-based control scheme, when using the commonly used Mean Absolute Value (MAV) and Logarithmic Variance (LogVar) feature, where the latter has shown linear properties [2].

METHODS AND MATERIAL

Surface EMG (sEMG) data was collected from seven able-bodied subjects. The subjects were instructed to performed four different hand gestures (flexion, extension, radial deviation and ulnar deviation), in three limb positions (down the side, lifted to the side, lifted forward). sEMG signals were recorded with Myo armband, positioned on the right forearm of the subjects while standing. The sEMG was recorded from eight channels with a 200Hz sample rate. Filtering was done with a second-order Butterworth high-pass filter ($f_c = 10\text{Hz}$).

Features were extracted using a window of 40 samples with 50% overlap. MAV represent the amplitude of the signal. It is defined as the average of the absolute values of the sEMG signal:

$$MAV = \frac{1}{N} \sum_{i=1}^N |x_i| \quad (1)$$

where N is the length of the signal, and x_i is the signal of i samples. LogVar is a nonlinear transformation of the variance:

$$\log(\sigma^2) = \log\left(\frac{\sum_{i=1}^N (x_i - \mu)^2}{N}\right) \quad (2)$$

where N is the length of the signal, x_i is the i^{th} sample of the signal and μ is the mean. PCA is applied to qualitatively determine the separability of the feature data. The regression models (regressors) are calculated as following:

$$Y = \alpha + \beta X \quad (3)$$

where Y is the estimated output, X is the extracted feature data, β is the regression coefficient, and α is the Y intercept.

One regressor was build for each wrist movement for each test subject: four for each feature. The offline regressor accuracy was tested qualitatively through superimposition of the output of the regressors build for each feature onto the actual data. The regressors were tested quantitatively by calculating the Root Mean Square Error (RMSE) between the expected movement and the regressor output. This was done for both training and test data to evaluate if the regressor had over- or under-fitted to the training data. The regressors were tested online in a virtual environment, where the time to complete a target-reaching task of sixteen targets was measured. The performance (time per reached target) of the online test was compared between the different limb positions of the same feature and between all limb positions of the two features through statistical analysis.

AIM

The aim for this project is expressed in the following hypothesis:

- It is possible to yield similar performance in different limb positions in myoelectric prosthetic control using a linear regression based control scheme.

ONLINE RESULTS

Results for the online test of regressor accuracy and control. The test is performed in a modified Fitts' Law test of reaching targets. The score is calculated as the relation between time and number of targets reached.

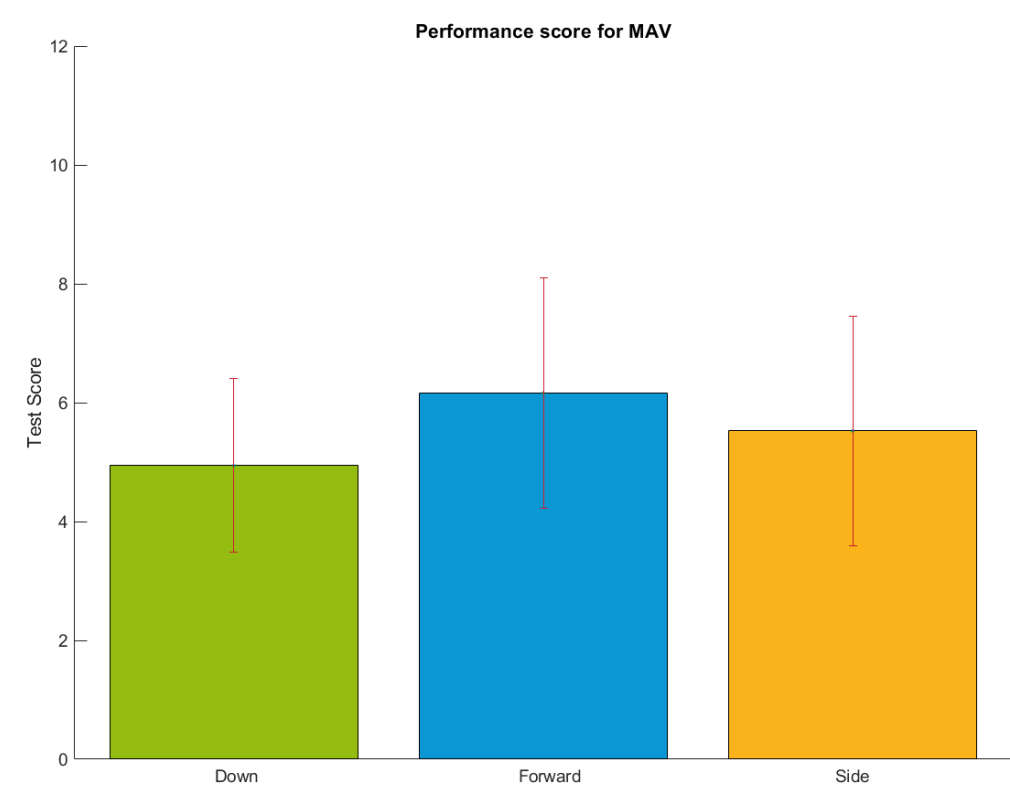


Figure 3: The mean test score among seven subjects when using regressors trained with MAV

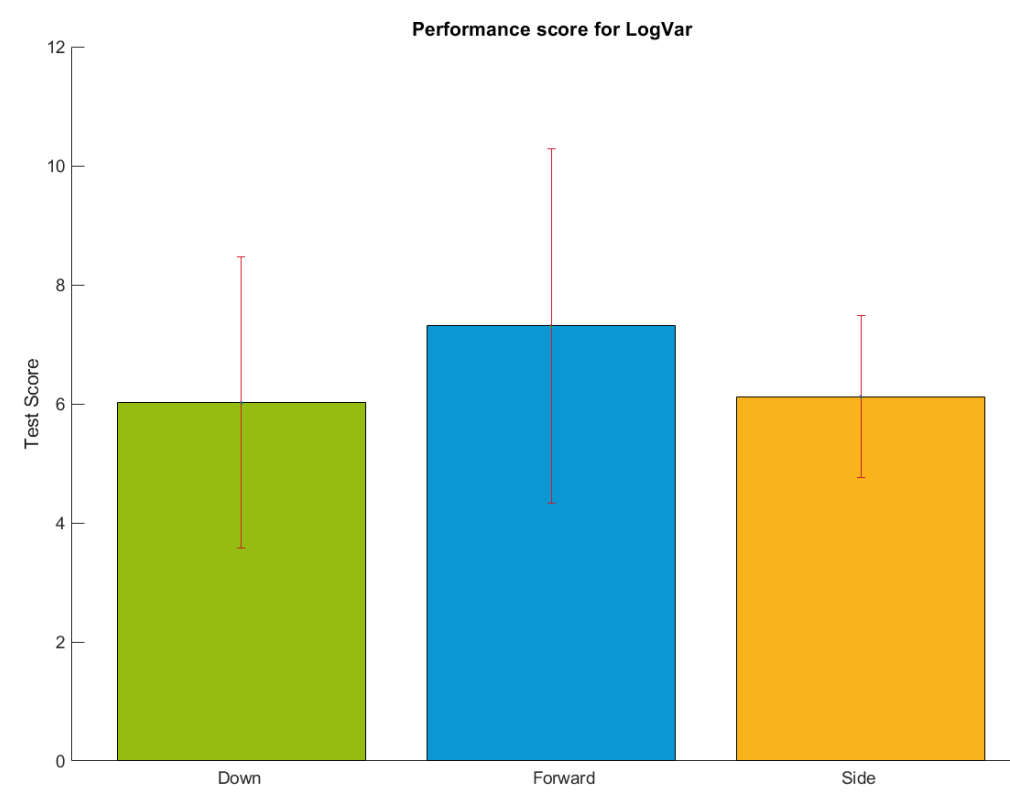


Figure 4: The mean test score among seven subjects when using regressors trained with LogVar

Using a Friedman's test the performance scores between the three limb positions prove not to be significantly different ($p = 0.5647$), when applying the LogVar trained regressors in the online test. For the MAV trained regressors the performance score between all limb positions cannot be proven significantly different either ($p = 0.1561$). There was no difference in the time to reach the targets across the two features (LogVar: 6.5 s, MAV: 5.5 s; $p = 0.13$).

REFERENCES

- [1] Anders Fougner, Erik Scheme, Adrian D.C. Chan, Kevin Englehart, and Øyvind Stavdahl. Resolving the limb position effect in myoelectric pattern recognition. *IEEE Transactions on Neural Systems and Rehabilitation Engineering*, 19, 2011.
- [2] J. M. Hahne, F. Biebmman, Ning Jiang, Hubertus Rehbaum, Dario Farina, F. C. Meinecke, K.-R Muller, and L. C. Parra. Linear and Nonlinear Regression Techniques for Simultaneous and Proportional Myoelectric Control. *IEEE Transactions on Neural Systems and Rehabilitation Engineering*, 22(2), 2014.
- [3] Han Jeong Hwang, Janne Mathias Hahne, and Klaus Robert Müller. Real-time robustness evaluation of regression based myoelectric control against arm position change and donning/doffing. *PLoS ONE*, 12(11):1–22, 2017.

OFFLINE RESULTS

Results of the superimposition of the regressor outputs on the estimated data.

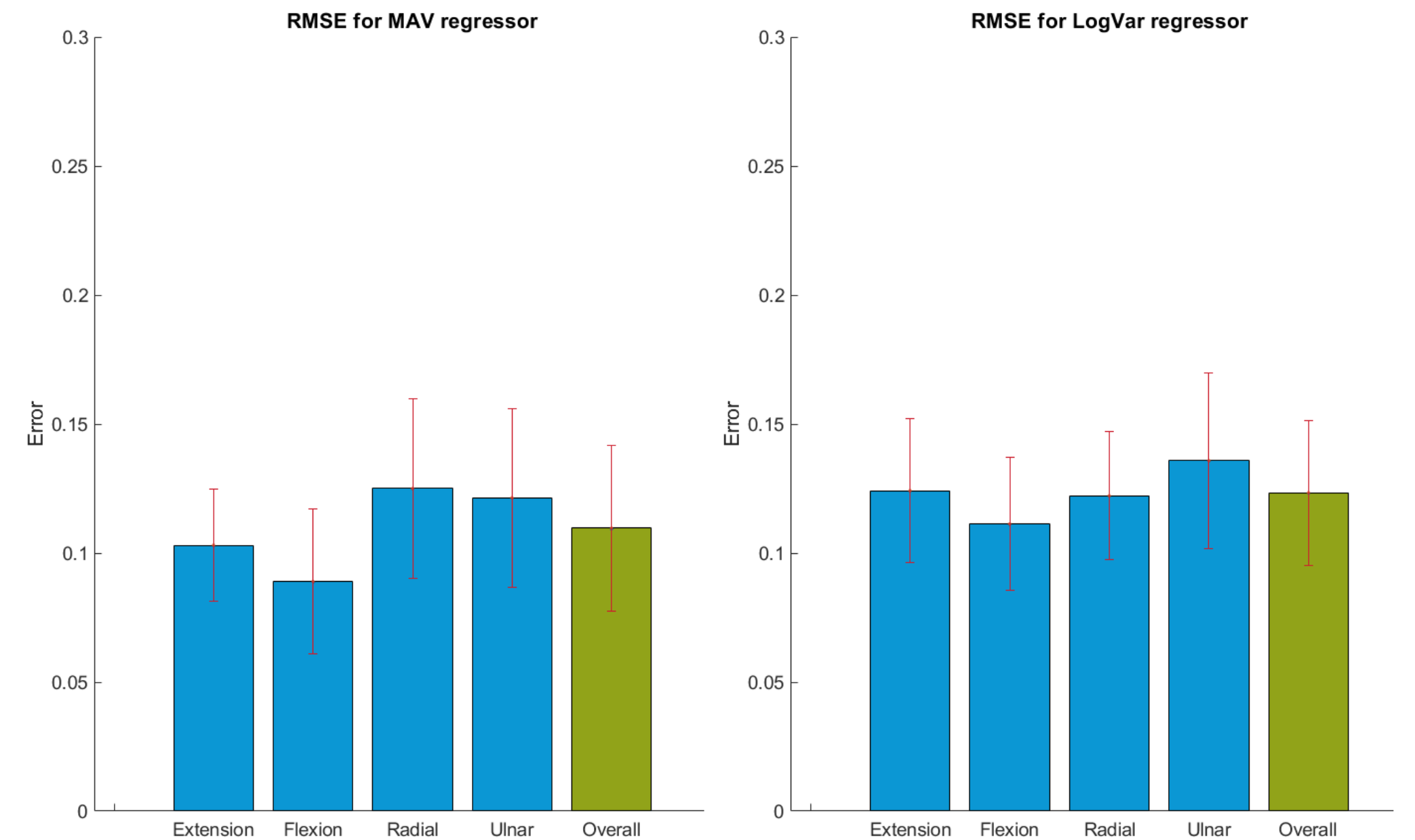


Figure 1: DATA

The results for the offline test of accuracy of the regressors of both test and training data. This test determines if the training of the regressors have over- or under-fitted to the training data.

Feature	Overall mean error	Highest mean error
MAV	0.0943 ± 0.0290	0.1088 ± 0.0366
LogVar	0.1107 ± 0.0298	0.1216 ± 0.0402

Table 1: RMSE of training data

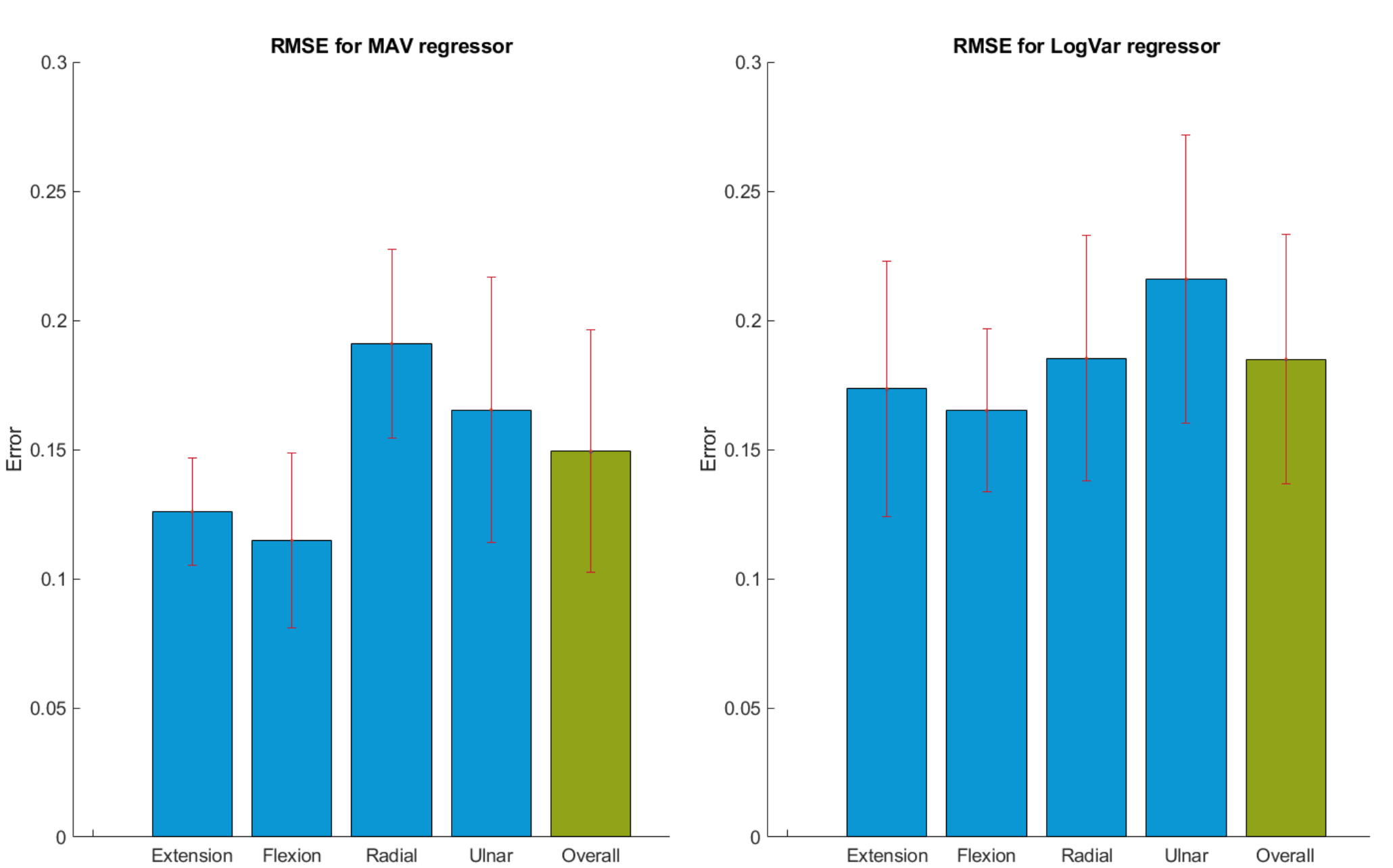
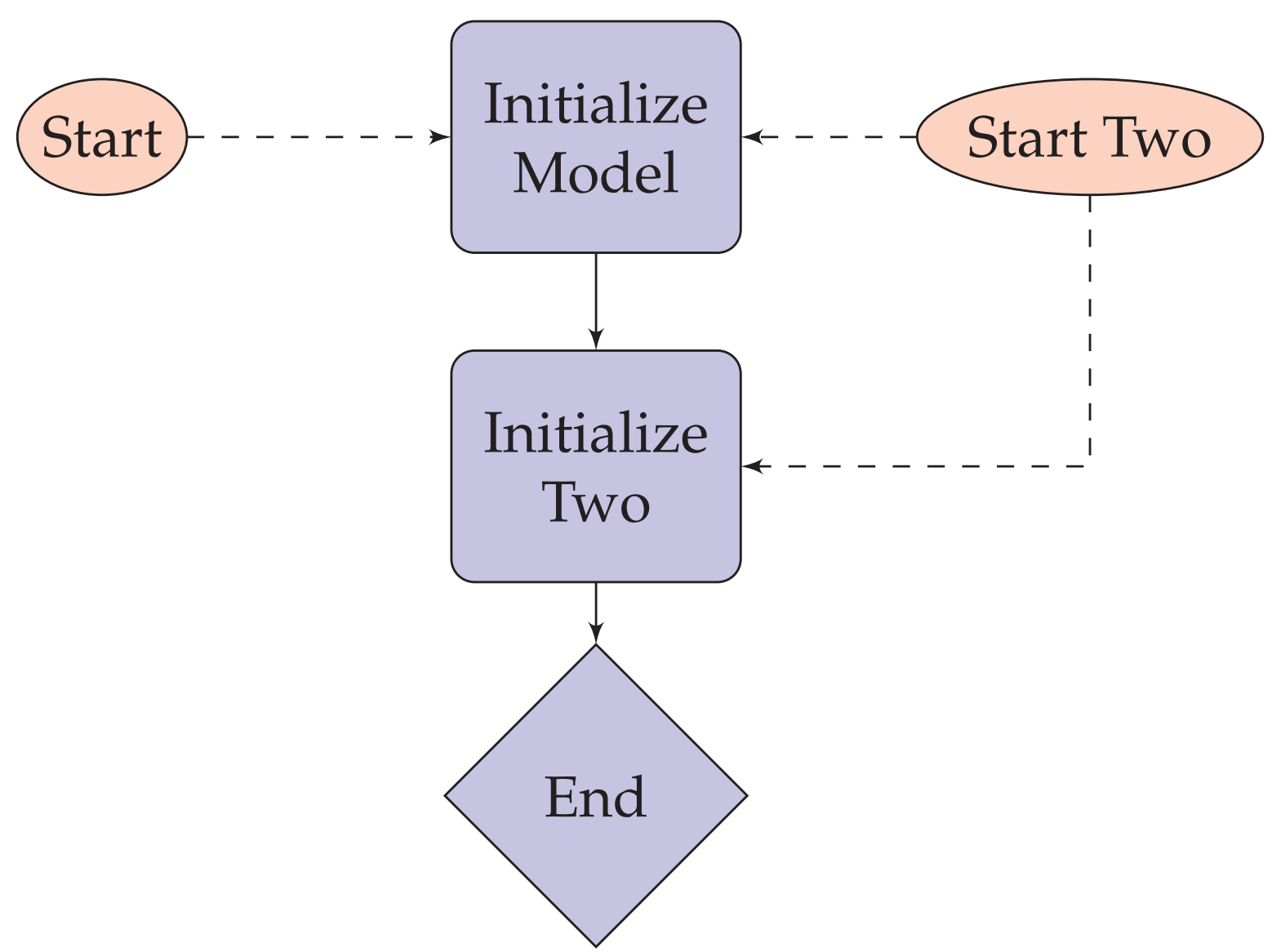


Figure 2: DATA

Feature	Overall mean error	Highest mean error
MAV	$??? \pm ???$	$??? \pm ???$
LogVar	$??? \pm ???$	$??? \pm ???$

Table 2: RMSE of test data

CONCLUSION



- Pellentesque eget orci eros. Fusce ultricies, tellus et pellentesque fringilla, ante massa luctus libero, quis tristique purus urna nec nibh. Phasellus fermentum rutrum elementum. Nam quis justo lectus.
- Vestibulum sem ante, hendrerit a gravida ac, blandit quis magna.
- Donec sem metus, facilisis at condimentum eget, vehicula ut massa. Morbi consequat, diam sed convallis tincidunt, arcu nunc.
- Nunc at convallis urna. isus ante. Pellentesque condimentum dui. Etiam sagittis purus non tellus tempor volutpat. Donec et dui non massa tristique adipiscing.

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