

Assessing Coordination of Advanced Dynamic Movements (in Patients with Motor Dysfunction (Following Stroke or Spinal Cord Injury))

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1 | Introduction

2 | Problem Analysis

2.1 Cardiovascular Diseases

Cardiovascular diseases (CVD) are the number one cause of death on a world wide scale. In 2015 CVDs was estimated to account for more than 31% of all deaths globally. [1] CVD are a collected term for a number of conditions revolving around diseases to the heart and system of blood vessels. According to the World Health Organisation (WHO) the top two causes of global deaths are the CVDs coronary artery disease and stroke. Of the two, stroke accounted for 10% of deaths in 2016. [2]

2.1.1 Stroke

A stroke is caused by either a blockage or rupture of blood vessels in the brain. As such stroke is divided into two subtypes; ischaemic stroke and haemorrhagic stroke. During a ischaemic stroke a blood vessel in the brain is blocked by blood cloths caught in narrow blood vessels. The narrowing of blood vessels are commonly caused by other conditions such as high cholesterol, high blood pressure, unhealthy lifestyle and ageing. If a blood vessel is blocked a part of the brain will be shot off from its blood supply. If not treated within minutes this can cause damage to brain cells in the cut-off area. [3, 4, 5] During an haemorrhagic stroke a blood vessel will rupture and blood will leak inside the brain. Depending on where in the brain the leak occurs the haemorrhagic stroke is either a intracerebral haemorrhage or and subarachnoid haemorrhage, intracerebral being inside the brain and subarachnoid occurring in the space between the brain and the cranium. In both types a rupture and leakage of blood can cause a sudden increase in pressure potentially causing damage to brain cells and can lead to sudden unconsciousness and death. The most common causes are high blood pressure, unhealthy lifestyle, diabetes and ageing. [3, 6, 5]

2.1.2 Stroke Complications

Complications following a stroke are common. In surviving patients 30-96% have been reported to experience post-stroke complications of both physical and psychological nature. Complications involve recurrent stroke and epileptic seizures, cardiac arrhythmias and failure, infections, problems in gastrointestinal and genitourinary systems, complication of immobility, dementia, pain and depression. [7] As so the consequences are many, however this study will focus on complications of mobility. Following a stroke complications related to movement are common. Depending on where in the brain the stroke occurs it can have a variety of outcomes that can affect the patients balance and motor control. Up to 38% of stroke patients have been reported to experience spasticity affecting the performance of dynamic muscle movements such as gait. Spasticity and motor control changes can occur following an upper motor neuron lesion. [7] Stroke patients are also at a higher risk of osteoporosis due to weakening of performing voluntary movements or movements as a whole if the patient experience hemiparesis [7].

2.2 Spinal Cord Injury

The spinal cord (SC) is part of the central nervous system (CNS) together with the brain. The SC is connecting the brain to the rest of the body by connecting to the peripheral nervous system (PNS). It is responsible for leading nerve impulses between the brain and body, to modulate movements, sensory inputs and visceral innervation. The SC extends from the brain just below the cranium down the spine to the lumbar vertebrae one and two (L1-L2). From L1-L2 to the end of the spine at the coccyx vertebrae or tailbone, bundles of nerve fibres extend further. The vertebrae bones encapsulates and protects the SC. However, trauma to the spine can cause trauma to the SC as well. [8]

The incidence for spinal cord injuries (SCI) ranges from 15 to 39 million a year in industrialized countries. Most traumatic causes are a result of traffic accidents, falls and violence. Causes for non-traumatic SCI are degenerative diseases and tumours. In prevalence of traumatic SCI, men outnumber women at a ratio of 3:1, while the prevalence is near equal in non-traumatic SCI. According to the National Spinal Cord Injury Statistical Center (NSCISC), the most frequent category for neurological damage is incomplete quadriplegia at 32.2% of cases. This is followed by complete paraplegia at 24.2%. Out of all SCI cases only 7.4% reach neurological recovery. [9]

2.2.1 Complications of SCI

Any injury to the SC causing neurological damage can lead to serious dysfunction depending on where the injury happens. This can lead to loss of sensory sensation and motor control and dysfunction to bladder, bowel and cardiovascular functions. [8] As mentioned earlier, this project will focus on complications of mobility. Many SCI patients experience rehospitization, depression and pain, following the injury. According to the NSCISC many patients are unsatisfied with their life in the years after injury. However, life satisfaction generally increase with years post injury. [9]

2.3 Rehabilitation

Patients suffering from neural damage caused by stroke or SCI will in many cases need to go through a rehabilitation process to regain or relearn lost functions [10, 11]. Currently many different methods for rehabilitation exist, many with focus on patients regaining control of limbs. Many patients suffer from loss of the ability to walk properly, as a result of losing control of the lower limbs. A giant step toward regaining autonomy and independence in daily life is to train patients balance and ability to walk again.

Rehabilitation programs for both stroke and SCI patients often involves training gait and the sensory-motor (SM) system in the brain. Studies have shown that due to neural plasticity patients can regain lost functions with training [12, 10]. Rehabilitation training functions through repetition of specific gait tasks while utilizing feedback to achieve improvements in gait coordination, speed and strength [12]. The training is often conducted using treadmills, on which

the patient will attempt to walk while being supported by an unloading harness. This training method can consist of both explicit and implicit methods; the explicit method is where patients will receive visual feedback to adjust the length of their steps in order to activate a cognitive process to adjust their gait. The implicit method will rely on resistance in order to train locomotion without the patient having to plan their step length. Another important aspect of rehabilitation of these individuals is their balance, and lately training of this ability has been shown to increase both speed and distance in walking tests. [10]

An important aspect of rehabilitation is that when assigning training to patients of stroke or SCI, it is important to evaluate the state of the patient, as different patients will have different levels of dysfunction depending on the severity of the damage caused by stroke or SCI. Rehabilitation should be suited to each patient individually. [10]

2.4 Assessing Gait in Rehabilitation

During rehabilitation patients must be assessed to evaluate the progressing of the rehabilitation process. Several different methods for assessing patient gait abilities have been developed to evaluate on the rehabilitation progress.

2.4.1 Measuring Gait in a Clinical Environment

Recent technological improvements makes it possible to perform advanced gait analysis (GA) while examining 3D kinematics and EMG in a clinical setting. This method provides the clinician with an advanced insight in the patients current abilities and gives the possibility of measuring and quantizing any changes that might occur during a rehabilitation process. [10]

The method of using 3D kinematics takes place in a laboratory with the use of cameras, surface electromyography (sEMG), force platforms and stereophotogrammetry equipment to provide the needed data to perform GA. The system provides recordings for qualitative analysis, as well as quantitative measures of muscle activation, contact forces with the ground and body position during gait. These measures are used to evaluate the gait cycle with regards to step length, cadence, swing time, rotation and power in the joints for the individual subject. [10]

An attempt to quantify the quality of gait with a single parameter was made with the Normalcy Index (NI), where the algorithm measures deviation of a patients gait pattern from the gait of healthy individuals through Principal Component Analysis (PCA). The mean pattern is based on some of the features obtained with GA. This method has been proven to be an effective tool to examine changes in gait over time. [10] Further advances in the quantification of the many features is the gait deviation index, the gait profile score and the movement deviation profile. All of these methods take different approaches to finding the deviation between healthy gait and the measured variables from the advanced clinical set-up described briefly above. [10]

Other approaches exist to measure improvement during rehabilitation. One study calculated the combined centre of pressure of the patient and a walking frame (WF) as a combined system, by measuring reaction forces of both the patient and the WF along with cameras capturing

the placement of the feet relative to the WF. This gave the possibility to calculate the weight supported through the frame and the stability of both patient and WF. [13]

2.4.2 Measuring Gait outside a Clinical Environment

Methods of measuring gait and other dynamic activities outside clinical environments are becoming more accessible and favourable over measurement methods bound to clinical environments. Rehabilitation and assessment in clinical environments rarely translate well to real life situations [14]. Such systems are most functional if they are wearable by the patient or test subject.

Wearable systems to analyse and monitor body dynamics are attracting an increased interest in research, where accelerometers and inertial measurement units (IMU) are the most used in newer studies. Here, studies have used wearable systems to measure upper limb kinematics and trunk posture, to evaluate on movement performance. [15] Wearable systems can also be used for assessing gait by implementing multiple sensors placed on the subjects lower limbs, measuring variables such as acceleration, gyroscopic, pressure forces and EMG depending on which system is implemented. Here, measuring forces applied to the feet can be done with force sensors based on either resistive, piezoelectric or capacitive designs, and often includes an implementation of these in shoes or insoles. [16] A study by Muro et al. [16] has been shown that the implementation into insoles reflects the measurements obtained from clinical motion analysis laboratories.

Inertial measurement units (IMU) can also be implemented in wearable devices. These consist of gyroscopes measuring the rotational inertia used to measure changes in direction, as well as accelerometers measuring the acceleration in three axes giving the opportunity to measure changes in balance or sudden knocks such as those experienced by the sensor while walking. [16]

A study by Hurwitz et al. [17], examined the importance of accelerometer position, age and walking speed on the accuracy of accelerometer based measurement of gait. It was found that the device location did not affect measures such as speed, cadence and single limb support time. Gait asymmetry and variability was shown to be affected by age and walking speed.

2.4.3 Shortcomings of Current Rehabilitation

It is known that clinical trials and training translates poorly to daily life outside clinical environments, however still current rehabilitation mainly perform training in clinical environments, or train tasks which poorly portrait normal daily life. [14] This is a problem since both stroke and SCI patients experience a greater risk of falls. The prevention of patients falling should be prioritized in rehabilitation as falls can lead to loss of independence and serious injury. Despite the consequences, studies have shown that 30-39% of stroke patients fall at least once during a rehabilitative process, and of these patients 42% experience multiple falls. [7, 18] According to a study by Wannapakhe et. al [19], out of a group of 100 SCI patients, 45 experienced falls

during a six month period post rehabilitation. Apart from the immediate risks and dangers to patients falling, falls can also further extend the rehabilitation period and worsen the rehabilitation of both motor and cognitive functions [20, 21]. This is a problem since strength recovery is usually greatest in the first 100 days following injury [8].

In addition, current rehabilitation programs still use qualitative methods for evaluating patients progress. These methods rely on the physician to evaluate how well the patient performs [22, 23]. This is a problem since qualitative evaluations are prone to changes from session to session depending on many factors which are not accounted for, like the patients level of energy or the physicians personal experience. This could be a problem since patients are observed to experience falls post rehabilitation [7, 18, 19]. This might suggest that current evaluation methods does not properly evaluate whether or not patients are fit for independent daily life.

2.4.4 New Methods for Balance and Gait Training

In contrast to current rehabilitation methods, mainly focusing on simple gait training, a rhythmic movement, newer approaches have begun to use dual-task training, incorporating cognitive tasks as well. Similarly, training involving advanced movements have suggested to improve balance for both stroke and Parkinson's disease patients [24, 25].

Studies have shown that dual-task mobility training helps improve balance and gait compared to groups that performed single-task training in stroke patients. The dual-task approach was designed to make the patient walk on a treadmill while performing either a cognitive or motor task at the same time. [26] The walking/motor dual-task method proved to be significantly better at improving speed, stride length and cadence for both dual-task and single-task tests. Combining walking and cognitive tasks improved the patients cadence and dynamic gait index, which describes balance while walking, in single-task tests. It was also found that combining balance and cognitive or motor tasks improved a number of balance measures significantly compared to single-task training. [26] Despite the outcomes reported in [26], the conclusion is that more studies are needed in order to support that dual-task training improves performance in dual-task tests. The review study shows that a dual-task approach improves single-task tests compared to the single-task training. [26]

A similar approach can be seen in studies where Tai Chi was used as a rehabilitation method for stroke and Parkinson's disease patients, implementing the aspect of thought and simultaneous movement into the training [24, 25]. This use of martial arts training resulted in multiple studies finding significantly higher improvement in balance compared to the control groups, while gait measures did not improve significantly with the implementation of Tai Chi training. [24] These findings can not lead to a final conclusion due to the number of trials and sample size, but the results indicate that martial arts could help increase balance in stroke patients [24]. It was also found that Tai Chi helps to reduce the number of falls for people suffering from balance problems after both stroke and Parkinson's disease, while in this study it did not result in a significant difference between balance measures compared with regular treatment [25]. It has also been found that Pilates training improves both static and dynamic balance in older adults

compared to the control group that only did their normal daily activities [27].

2.5 Problem definition

The previous chapter introduces the problem of patients suffering from complication of mobility caused by stroke or SCI and leads to the current rehabilitating methods used to train patients to regain mobility. However, these methods are not standardised and evaluations of patient performance is subjected to physicians personal experience and patients immediate feeling. Additionally, most evaluations occur in clinical environments when performing simple movement tasks, which translate poorly to real life.

It can be discussed whether or not current rehabilitation training with single-task training of simple movements is properly prepares patients to live independent daily lives post rehabilitation. This project propose that training involving advanced dynamic movements can further improve on patients strength and balance, better preparing them for daily life, when compared to traditional simple movement training. However, there exist no suitable system to evaluate advanced dynamic movements. Thus a new system is needed to have a way to measure and assess patients ability to perform advanced dynamic movements to determine if this type of training is an improvement to current rehabilitation methods.

1. How is it possible to develop a wearable system to measure performance of advanced dynamic movements to evaluate a subjects performance in relation to balance, coordination and sequence of execution.
2. How is it possible to develop a wearable system to evaluate subjects Centre of Pressure when performing advanced dynamic movements.
3. How can a wearable system be developed which can measure Centre of Pressure and rotational forces of advanced dynamic movements to assess coordination control and balance.
4. How can a wearable system be developed which can be used to assess coordination control and balance of advanced dynamic movements.
5. Evaluating Centre of Pressure/Balance in subjects performing the karate kata Pinan Nidan. A proof of concept study.

3 | Methods

For this project reaction and pressure forces are collected from subjects performing the karate kata Pinan Nidan. A karate kata is a sequence of detailed choreographed patterns of movements. Many different types of kata exist, each practice visualisation, balance and basic technique through repetition of movements. Different katas have different sequences of movements, some are more difficult than others where jumps and kicks are part of the movements. For this projects data acquisition the kata Pinan Nidan is chosen. Pinan Nidan consists of a series of movements involving steps, turning and hand strikes, where the performers' feet are on the ground at most times. Pinan Nidan takes between 30 and 60 seconds to perform depending on the speed of movements. The kata consists of 13 stepping, 11 turning, 7 punching and 13 blocking movements. [28, 29, 30]

3.0.1 Subjects

For this project three healthy test subjects will be used; one who is a master at karate (+30 years of karate experience), one intermediate (3-5 years karate experience) and one novice (less than 1 year of karate experience). All subjects are able-bodied and have no neurological or muscular injuries. Subjects were prior to the test instructed about the purpose of the study and their role as test subjects.

3.1 Instrumentation

For this project data will be acquired using gyroscopes and force sensors. The gyroscopes are provided through the use of the Shimmer3 device from Shimmer Sensing (Dublin, Ireland)). Force sensors are from Interlink Electronics Inc. (California, USA) of the 400 Series.

The Shimmer3 device is a nine degree of freedom (DoF) Inertial Measurement Unit (IMU) possessing four different types of sensors; accelerometer, gyroscope, magnetometer and altimeter. The Shimmer3 is capable of being configured to enable or disable specific sensors depending on which is needed. For this project only the gyroscope module of the device will be used. The gyroscope is a MPU-9150, with a range of ± 250 / ± 500 / ± 1000 / ± 2000 degrees per second (dps). The gyroscope has sensitivity of 131 LSB/dps at ± 250 dps. [31] Communication between the Shimmer3 devices and the computer is through Bluetooth (Bluetooth SIG, Washington, USA). The computer will be running MATLAB (MathWorks, Inc. Massachusetts, USA) and the *Shimmer MATLAB Instrument Driver Library* to collect the streamed data from the Shimmer3 device. The Shimmer3 device has dimensions of 51mm x 34mm x 41mm and is easy to place nearly anywhere on the body with elastic straps with snap clips. Two Shimmer3 devices will be used for this project.

The force sensors used in this project are Force Sensing Resistors (FSR) from Interlink Electronics, models 402 and 406. The FSR 402 is a 13mm diameter circle single-zone resistor

capable of force detection in a range from 20g to 2kg. The FSR 406 is similar but covers a larger square area of 38mm \times 38mm. [32] A total of six sensors will be used with three sensors under each foot. An Arduino Uno will be used for handling recording and saving the data from the FSRs. The Arduino Uno is mounted on a breadboard, and connected to six jack stick plugs, an microSD card reader and batteries for power supply (see figure 3.1). The FSRs are connected to the Arduino through 3.5mm jack sticks. Data collection is initiated by pressing a designated record button. When recording is active a LED on the board will light up. Data from the FSRs will be stored on a microSD card and be processed offline with MATLAB.

The system setup as a whole for both the gyroscope and FSR parts can be seen illustrated in a block diagram on figure 3.1.

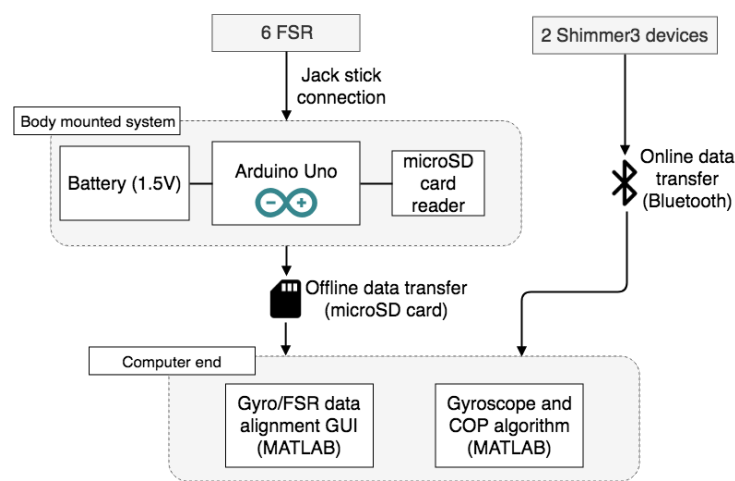


Figure 3.1: Block diagram of the system. The left side is of the pressure sensing part utilizing the FSRs. On the right side is the Shimmer3 devices (gyroscopes). All data is collected and processed on a computer using MATLAB.

3.1.1 Instrumentation placement

During data acquisition the subjects will be wearing the instruments presented earlier in section 3.1. The Shimmer3 devices will be placed, one on each leg, lateral distal to the knees of the subject.

The FSRs will be placed on the sole of each foot of the subject. One FSR 406 is placed at the lateral eminence of the sole. Of the two FSR 402 sensors, one will be placed under the heel and the other medial eminence of the sole. The placement of FSRs can be seen on figure 3.2.

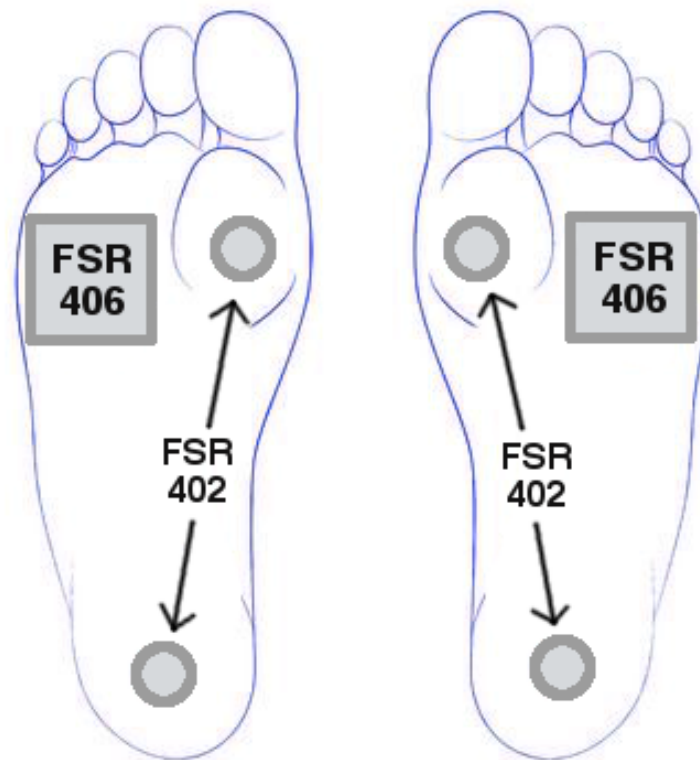


Figure 3.2: The placement of the FSR 402s and 406 under the foot of subjects.

The Arduino-setup will be placed at the lower back of the subject and handle data collection. Collected data will be stored on an microSD card for offline analysis with MATLAB. An illustration of device placement on a subject can be seen in figure 3.3.

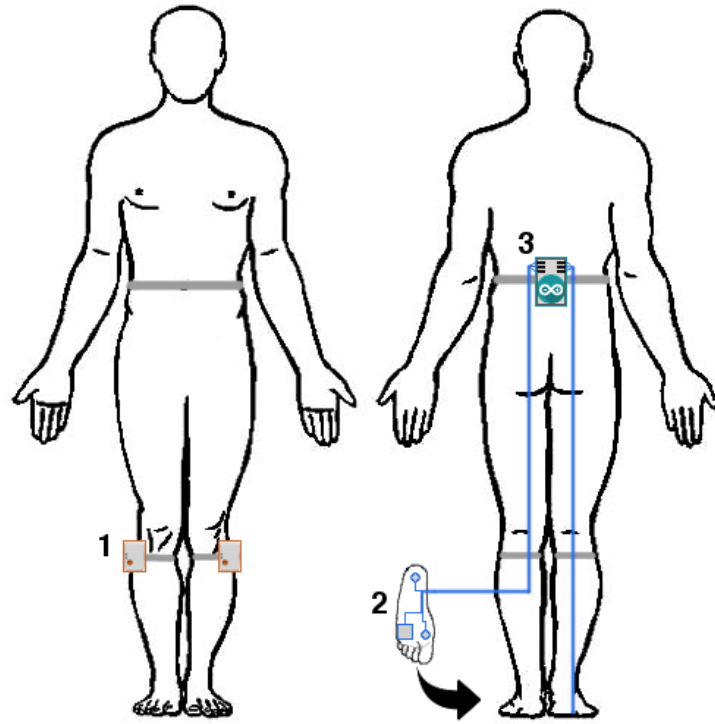


Figure 3.3: The placement of the Shimmer3 IMU devices (1), FSRs under to feet (2) and Arduino-setup (3) on a test subject.

3.2 Data Acquisition

Data acquisition from both the FSR sensors and the Shimmer3 devices are set to have a sample frequency of 100Hz. This sample rate is used by others performing similar measurements [33, 34, 35]. Additionally, the sample rate is decided to be the same so it is possible to match the two data streams to each other, so it is possible to compare measured pressure forces under the feet while matching it to movement of the body. A simple graphical user interface (GUI) have been developed to match the data. This manual approach is favourable for this project as it were determined that it would be more time consuming to develop an algorithm to automatically match data streams. It would also go beyond the scope for the project.

Data from the Shimmer3 devices are send and saved directly to MATLAB via Bluetooth and stored in $n \times 3$ matrices, one for each leg.

For saving acquired data from the FSR sensors an Arduino program have been written to arrange measurements into an $n \times 6$ matrix. Each column corresponds with the channel input for each FSR. See figure 3.4 for the numbering of FSRs and channels. Rows in the matrix are time steps. The data is saved to a *.txt*-file on the microSD card.

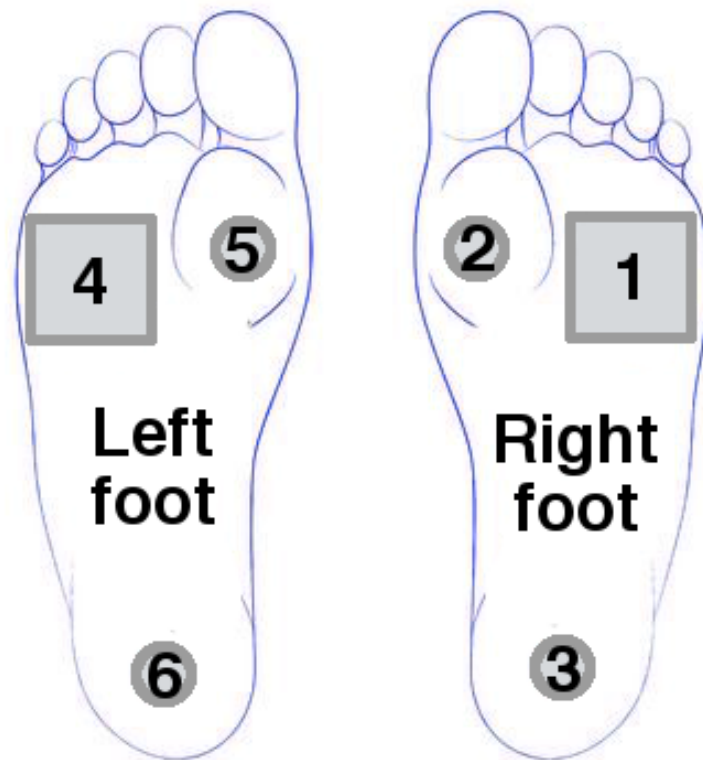


Figure 3.4: The numbering of each FSR sensor according to the channel they are recorded to in the Arduino program.

3.3 Data Analysis / Processing

This section covers processing and analysis of acquired data. All data processing is performed using MATLAB.

3.3.1 Filtering

The spectral density of gyroscope data have been analysed to investigate frequencies of interest. From the Fourier transform (FT) of gyroscope data (see figure 3.5) it can be observed that frequencies over 10Hz contain very little information. To avoid possible noise and artefacts a third order Butterworth filter have been implemented with a cut off frequency at 25Hz. This filter order and cut off frequency is decided ??

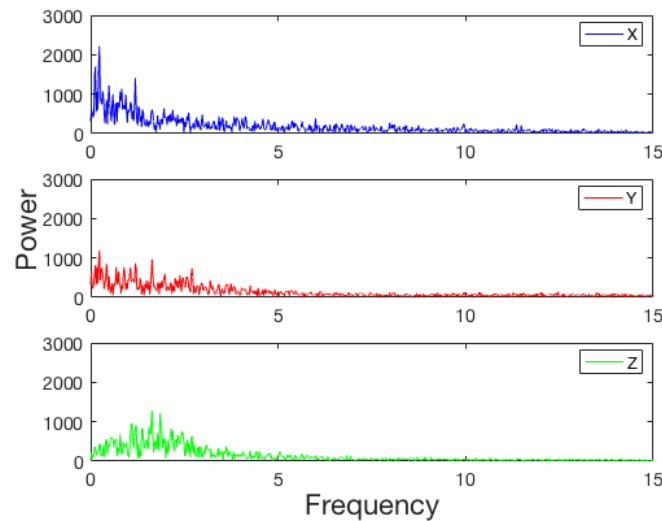


Figure 3.5: The power spectral density of gyroscope data from the left leg of one subject.

3.3.2 Data Alignment

Because the measurements from the FSRs are run on an Arduino, and the gyroscopes run through a Shimmer Sensing developed script for MATLAB, the timing for the measurements are run differently. In order to analyse FSR data to the corresponding time for gyroscope data a data alignment GUI have been developed in MATLAB. The implemented alignment program is a simple GUI which creates a plot where different channels from the six FSRs and six DoFs from the gyroscopes (three for each on each leg) can be shown or hidden. Additionally each channel can be translated left or right. This enables to align data from the FSRs to the gyroscopes, based on a spike in measurements caused by a small jump subjects will be asked to perform before and after performance of Pinan Nidan. An example of the alignment GUI can be seen in figure 3.6.

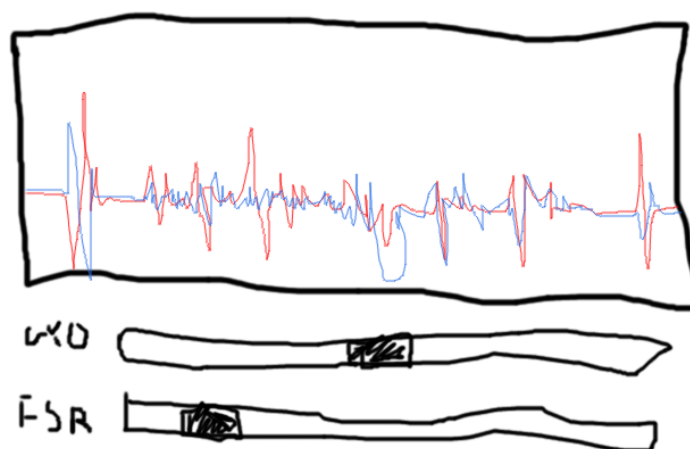


Figure 3.6: The alignment GUI showing a selected number of channels from the FSRs and gyroscopes. All channels can be translated in order to align timestamps for the FSR measurements to timestamps for the gyroscopes.

3.3.3 Calculation of Centre of Pressure

MATLAB COP code description

3.4 System test

This section covers the test of the system, prior to conducting the experiment for the project.

3.4.1 Method of test for gyroscopes

The authors assess that a test of the gyroscopes is not necessary, as the Shimmer3 devices will be calibrated using the built in function of Shimmer Sensing's program, Consensys, to ensure the devices are working as expected.

3.4.2 Method of test for Force Sensitive Resistors

The FSRs will be tested by placing a 1kg weight covering a surface area of "insert cm2" applied in the middle of both types of FSRs. This is done to test if any of the sensors are broken or deviate compared to the other FSRs.

3.4.3 Test results for Force Sensitive Resistors

A weight of 1kg were applied to each FSR in order from FSR channel 1 to 6. The weight were applied for approximately 5 seconds to each FSR in the middle of the sensor area. Results of the test of the FSRs is shown in figure 3.7.

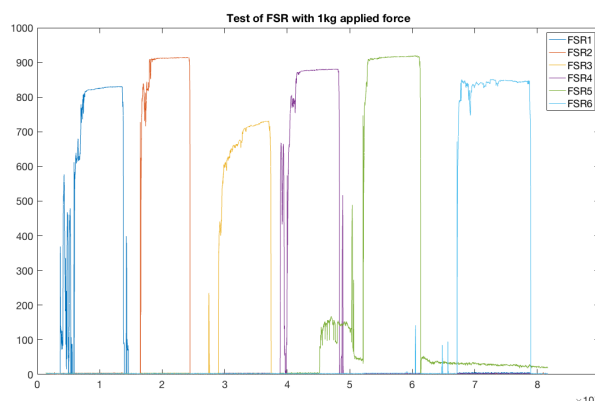


Figure 3.7: The result of the test of the 6 FSRs.

As it "might" can be seen from the results of the FSR test, FSR number 3, located at the heel of the right foot, returns a lower resistance when applied a 1kg weight compared to the other FSRs.

The authors learned too late in the work period that one of the FSRs were returning resistance varying from the other FSRs. This was not anticipated and no replacement had been ordered. However, the authors hope/judge/evaluate that the FSR will not affect the data processing the calculations of Centre of Pressure (COP) too much.

During continuous testing of the system during development the authors experienced damage to one of the FSRs, and are at this point in the work, unable to obtain a replacement. However, as this project is mainly to function as a proof of concept work, the authors determine that one sensor should not affect

3.4.4 System test

The system as a whole will be tested with a walk sequence. The sequence will involve periods of no movement, movement by walking and turning and a light jump to mark the beginning and end of the sequence. The walk sequence is as follows:

- 5 second pause
- Light jump
- 5 second pause
- Walk five steps
- 180 degree turn
- Walk five steps
- 5 second pause
- Light jump
- 5 second pause

Following the system test the acquired data will be qualitatively evaluated to ensure everything works as intended.

3.4.5 Test results for System test

Everything was fine. maybe.

3.5 Protocol

3.5.1 Aim

The experiment aims to measure the ground reaction forces during the performance of the karate kata Pinan Nidan. At the same time gyroscopic sensors will measure the rotational forces of the legs for later use in data analysis.

3.5.2 Design

Before the experiment

- The data file “DATA.txt” on the microSD card for the Arduino will be emptied and the microSD card will then be placed in the Arduino-setup.
- Subjects have knowledge and various amounts of experience with the kata Pinan Nidan prior to the experiment. No subject needs instruction of performance of the kata.
- The subject is instructed that before recordings of the kata they will stand still for five seconds, do a small jump and stand still for five seconds. This small sequence is to be performed both before and after performance of the kata.

Initial part

1. The person responsible for the test will mount the force sensors underneath the feet of the subject according to the labelling on the sensors. These sensors will be placed as following on both feet:
 - One FSR406 sensor on the lateral eminence of the sole
 - One FSR402 sensor on the medial eminence of the sole
 - One FSR402 sensor at the heel
2. The distance between the sensors will be measured for later use.
3. 1 Shimmer3 device (gyroscopes) will be mounted lateral distal to the knee. One sensor on each leg.
4. The Arduino-setup will be mounted around the waist, and the system will be placed at the lower back.
5. Elastic straps will be mounted right above the knee to ensure the cables for the force sensors stays in place, and to mount the Shimmer3 devices.
6. The force sensors will be plugged into the Arduino-setup according to the numbering on both the system and the sensor cables.
7. Shimmer3 devices will be connected to MATLAB.
8. The subject will practice one round of Pinan Nidan to warm up.
9. The subject stands ready to begin performing Pinan Nidan with recordings.

Data acquisition part

1. Recording from the Shimmer3 devices will be initiated in MATLAB.
2. The Arduino system will be powered up and recording started by pressing the designated “Record” button until the red LED lights up.
3. Subject will be asked to stand still for 5 seconds then do a small jump, stand still for 5 seconds, do another small jump and then stand still for 5 seconds before moving on.
4. After this initial movement, the subject will be asked to perform the Pinan Nidan.
5. When the subject is done with the Pinan Nidan, they will be asked to perform a 5 second pause, small jump and 5 second pause again.
6. The recording is stopped by pressing the “Record” button until the red LED turns off. The Arduino-setup will be shut off and the microSD card removed from the setup to extract the data to a computer.
7. After data is transferred to the computer, the microSD card is inserted to the Arduino-setup, and the process continues from step 1 in “Data acquisition part”.

The subject will perform Pinan Nidan four times in total, one for practice and three were data is acquired.

Removal of the system

1. After the data acquisition the subject will be asked to stand still and the Shimmer data-stream will be stopped.
2. At the same time the “Record” button on the Arduino will be pressed until the red LED turns of.
3. The Arduino-system will be turned off and all the sensors and the Arduino will be removed from the subject.

3.5.3 Participants and statistical considerations

The included three participants are selected based on their experience with the kata Pinan Nidan. This includes a master (+30 years of karate experience), intermediate (3-5 years of karate experience) and novice (less than 1 year of karate experience) The number of participants is chosen as the study doesn’t aim to find a statistical significant difference between the subjects, but rather aim to examine if there’s a way to determine the stability of the subjects during the Pinan Nidan.

The time for the experiment will be 45-60 minutes.

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