

# Cryo-EM Reconstruction of Continuous Heterogeneity by Laplacian Spectral Volumes

Group Meeting

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## Cryo-EM reconstruction of continuous heterogeneity by Laplacian spectral volumes

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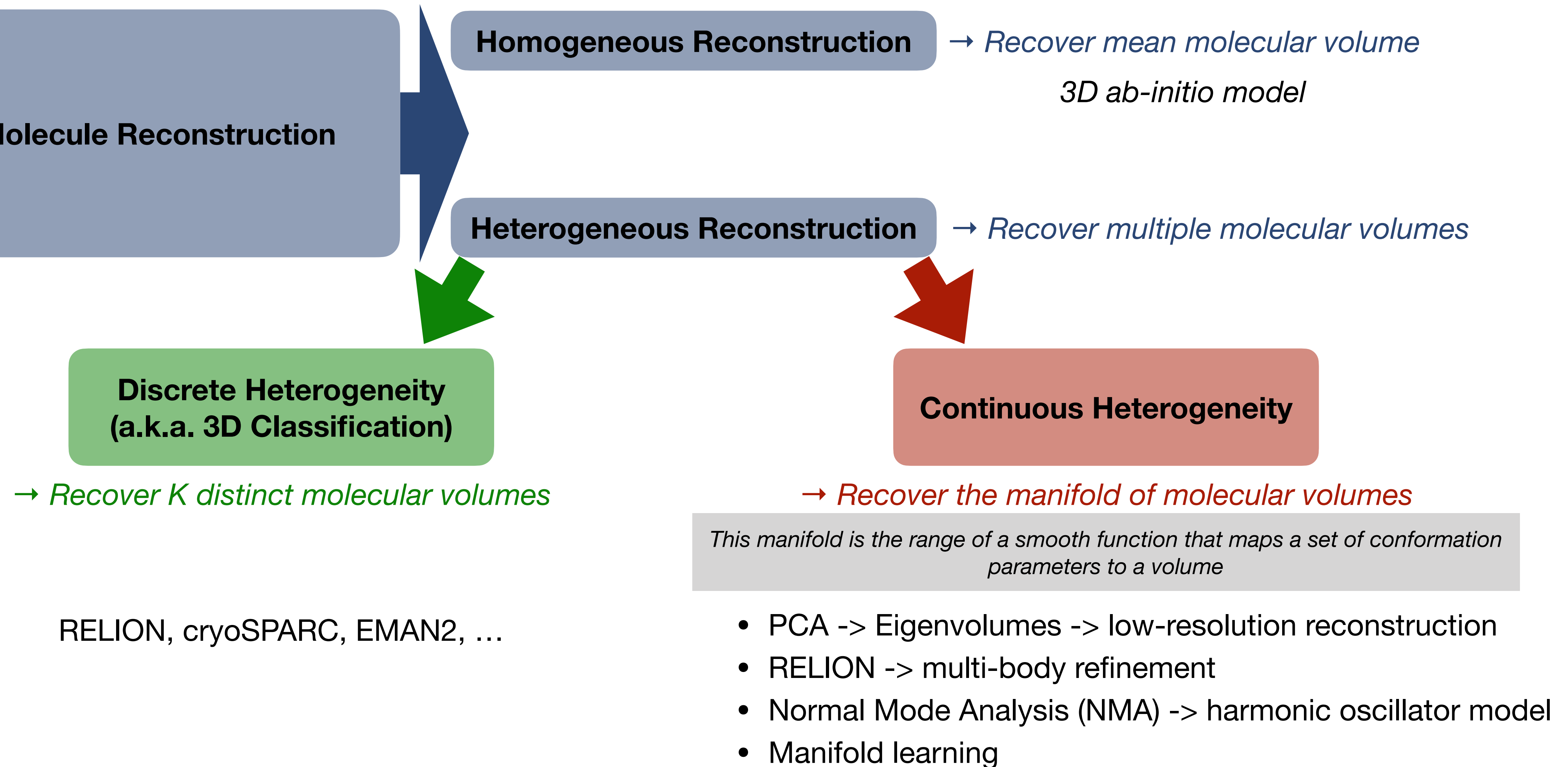
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# Reconstruction of Non-rigid Molecules



# Problem Formulation — Forward Model

- The individual particle images are formed by:

$$\mathbf{y}_s = P_s \mathbf{x}_s + \epsilon_s \quad \forall s = 1, 2, \dots, n$$

Volume rotation operator  $R_s$  convolution with a point spread function  $\mathbf{h}_s$

- Molecular volumes:  $\mathbf{x}_1, \dots, \mathbf{x}_n \in \mathbb{R}^{N^3}$
- Particle images:  $\mathbf{y}_1, \dots, \mathbf{y}_n \in \mathbb{R}^{N^2}$
- Noise:  $\epsilon \sim \mathcal{N}(0, \sigma^2 \mathbf{I}_{N \times N})$
- Linear imaging operators:  $P_1, \dots, P_n \in \mathbb{R}^{N^2 \times N^3}$

To define the imaging operator, one must incorporate an **interpolation** scheme since the volumes lie on a discrete grid  
→ express tomographic projection in the **Fourier domain**

- Discrete Fourier transform is given by:

$$(\mathcal{F}_d \mathbf{s})(\mathbf{k}) := \sum_{\mathbf{u} \in M_N^d} e^{-2\pi i \langle \mathbf{k}, \mathbf{u} \rangle} \mathbf{s}[\mathbf{u}] \quad \forall \mathbf{k} \in \mathbb{R}^d$$

- $\mathbf{k}$  : wave vector
- $\mathbf{u}$  : voxel index
- $\mathbf{s}$  : d-dimensional signal

- Using the **Fourier slice theorem** to express the projection image in the Fourier domain as follows:

$$(\mathcal{F}_2 P_s \mathbf{x}_s)([k_1, k_2]^T) = (\mathcal{F}_3 \mathbf{x}_s)(R_s^{-1}[k_1, k_2, 0]^T) \cdot (\mathcal{F}_2 \mathbf{h}_s)([k_1, k_2]^T)$$

Contrast transfer function (CTF)

# Problem Formulation — Inverse Problem

- Homogeneous case ( consider mean volume  $\boldsymbol{\mu} \in \mathbb{R}^{N^3}$  ):

$$\mathbf{y}_s = P_s \boldsymbol{\mu} + \epsilon_s \quad \forall s = 1, 2, \dots, n$$

$$\hat{\boldsymbol{\mu}} = \arg \min_{\boldsymbol{\mu}} \sum_{s=1}^n \left\| \mathbf{y}_s - P_s \boldsymbol{\mu} \right\|^2$$

- Continuous heterogeneity:

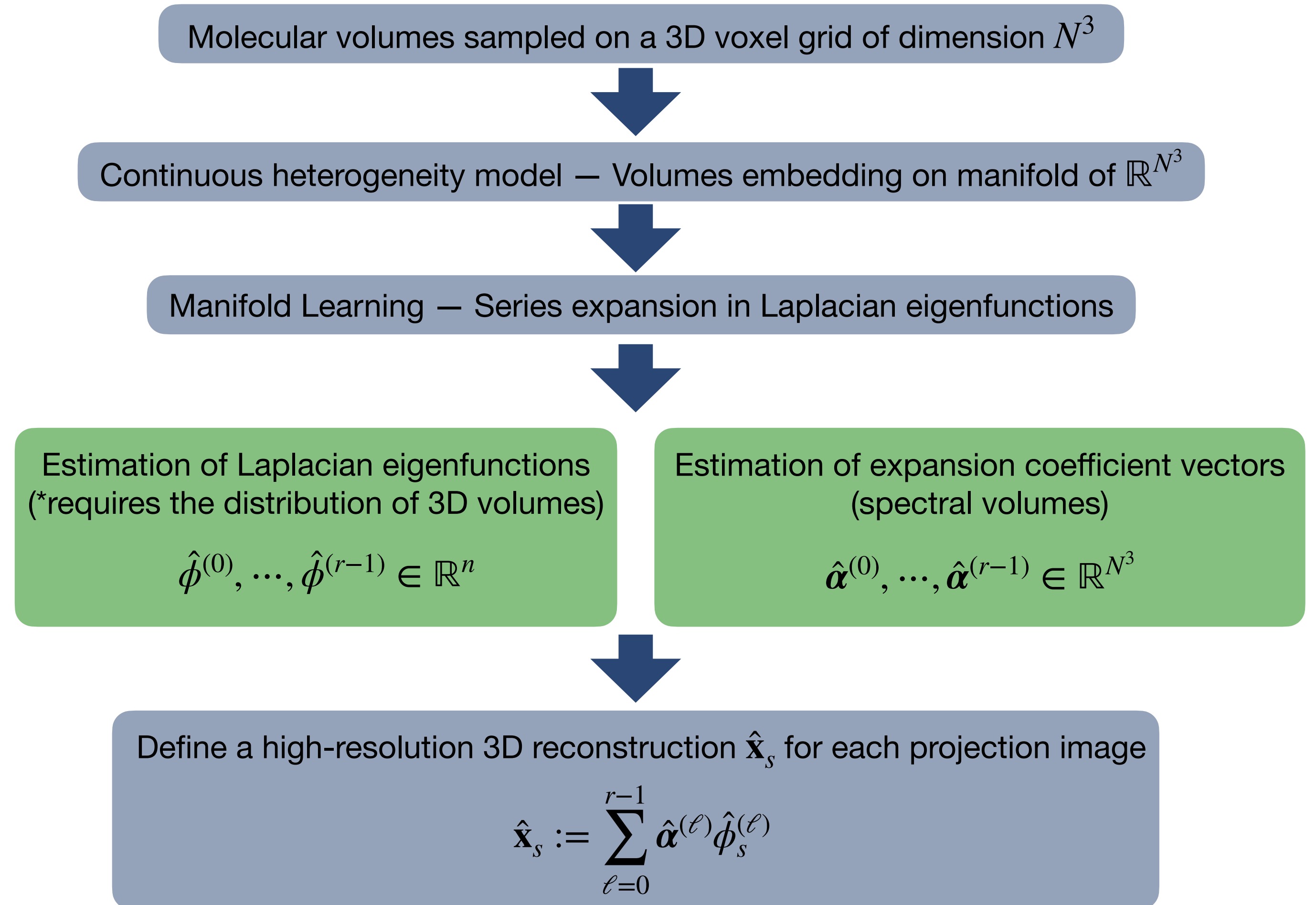
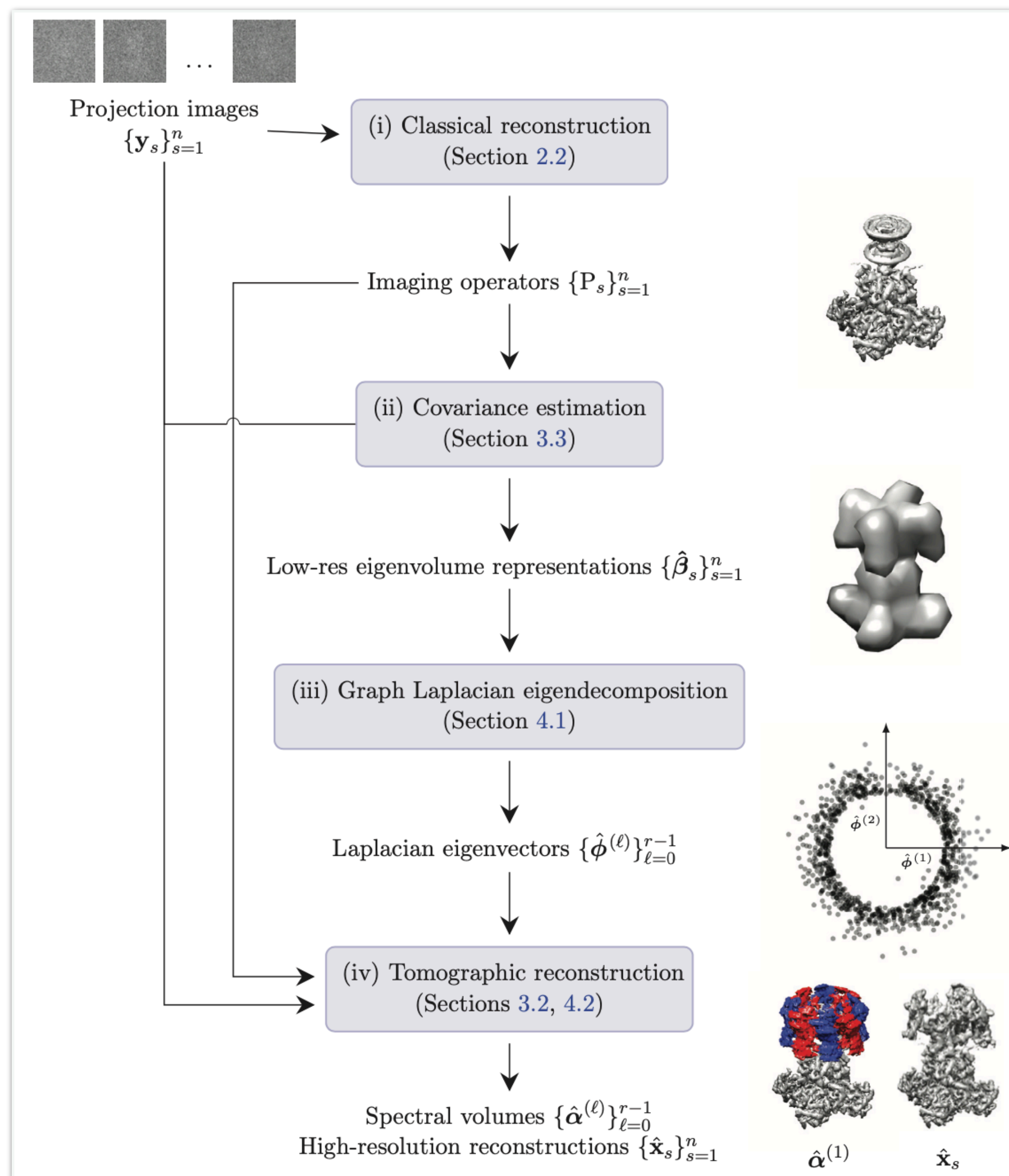
$$\mathbf{y}_s = P_s \mathbf{x}_s + \epsilon_s \quad \forall s = 1, 2, \dots, n$$

$$\hat{\mathbf{x}}_s = ?$$

- Two main assumptions made in this paper:
  - ▶ The molecular volumes in the sample lie near **a low-dimensional manifold**.
  - ▶ The imaging operators can be **accurately estimated** using standard cryo-EM reconstruction tools.



# Pipeline of Method from this Paper



# Low-Resolution Reconstruction

- Covariance estimation: each reconstructed volume is a linear combination of  $q$  **PCA eigenvolumes**  $\Rightarrow \hat{\mu} + \hat{V}_q \hat{\beta}_s$
- Defines some mapping  $(\mathbf{y}_s, P_s) \mapsto \beta_s$  where  $\beta_s \in \mathbb{R}^q$  is the vector of eigenvolume coefficients corresponding to a low-dimensional representation of  $\mathbf{x}_s$
- Ignore potential ambiguities due to the projection and consider the low-resolution reconstruction as a linear dimensionality reduction of the underlying volume  $\mathbf{x}_s \mapsto \beta_s$

# Manifold Spectral Representation

- Approximation of molecular volumes using an orthogonal basis expansion of first  $r$  Laplacian eigenfunctions:

$$\mathbf{x} \approx \sum_{\ell=0}^{r-1} \alpha^{(\ell)} \phi^{(\ell)}(\beta(\mathbf{x})) \quad \forall \beta \in \mathbf{B}$$

Spectral volumes      Laplacian eigenfunctions:  $\mathbf{B} \mapsto \mathbb{R}$

- Spectral volumes:  $\alpha^{(0)}, \dots, \alpha^{(r-1)} \in \mathbb{R}^{N^3}$
- Image of  $\mathbf{x}$  in PCA coordinates:  $\beta(\mathbf{x}) \in \mathbf{B}$

- Employ **Laplacian eigenmap** from the field of manifold learning to obtain estimates:

$$\hat{\phi}^{(0)}, \dots, \hat{\phi}^{(r-1)} \in \mathbb{R}^n$$

→ Build a **weighted undirected graph**, where the vertices correspond to the projection images  $\mathbf{y}_1, \dots, \mathbf{y}_n$  and the edge weights  $W_{ij}$  are estimates of the affinity between the underlying molecular conformations.

Gaussian kernel weight:  $W_{ij} = e^{\frac{-\|\hat{\beta}_i - \hat{\beta}_j\|^2}{2\sigma^2}}$

- A data-driven variant of the spectral expansion:

$$\mathbf{x}_s \approx \sqrt{n} \sum_{\ell=0}^{r-1} \alpha^{(\ell)} \hat{\phi}_s^{(\ell)} \quad \forall s = 1, 2, \dots, n$$

$\sqrt{n}$  factor is needed for normalization:  $\sum_{s=1}^n \left( \hat{\phi}_s^{(\ell)} \right)^2 = 1$



# Generalized Tomographic Reconstruction

- Applying the imaging matrix  $P_s$  for the spectral expansion and plugging in the forward model:

$$\mathbf{y}_s \approx \sqrt{n} \sum_{\ell=0}^{r-1} (P_s \boldsymbol{\alpha}^{(\ell)}) \hat{\phi}_s^{(\ell)}, \quad \forall s = 1, 2, \dots, n$$

- Seek spectral volumes  $\hat{\boldsymbol{\alpha}}^{(0)}, \dots, \hat{\boldsymbol{\alpha}}^{(r-1)}$  that minimize the squared error:

$$(\hat{\boldsymbol{\alpha}}^{(0)}, \dots, \hat{\boldsymbol{\alpha}}^{(r-1)}) := \arg \min_{\boldsymbol{\alpha}} \sum_{s=1}^n \left\| \mathbf{y}_s - \sqrt{n} \sum_{\ell=0}^{r-1} (P_s \boldsymbol{\alpha}^{(\ell)}) \hat{\phi}_s^{(\ell)} \right\|^2$$

- The high-resolution reconstructions of the molecular volumes are now given by:

$$\hat{\mathbf{x}}_s = \sqrt{n} \sum_{\ell=0}^{r-1} \hat{\boldsymbol{\alpha}}^{(\ell)} \hat{\phi}_s^{(\ell)}, \quad \forall s = 1, 2, \dots, n$$



*This estimator generalizes the least-squares estimator from **a single mean volume**  $\hat{\mu}$  to **multiple volumes**  $\hat{\boldsymbol{\alpha}}^{(0)}, \dots, \hat{\boldsymbol{\alpha}}^{(r-1)}$  whose contribution to the reconstructed volumes is given by the **Laplacian eigenvectors**  $\hat{\phi}^{(0)}, \dots, \hat{\phi}^{(r-1)}$*

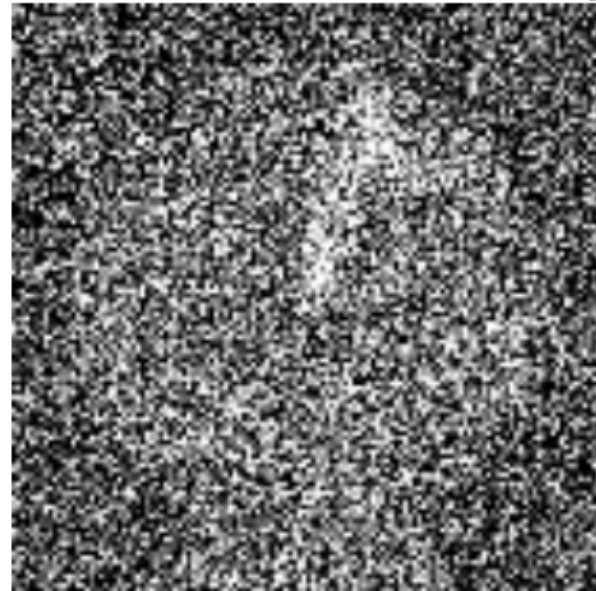


# Result — 2D/3D Clock Face Dataset

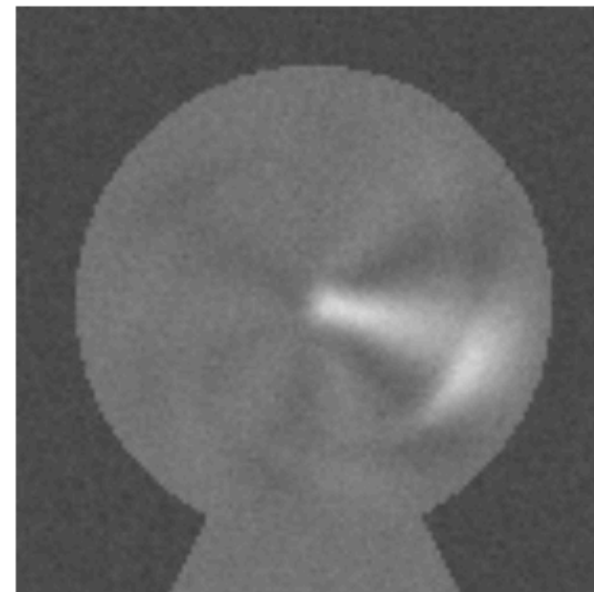
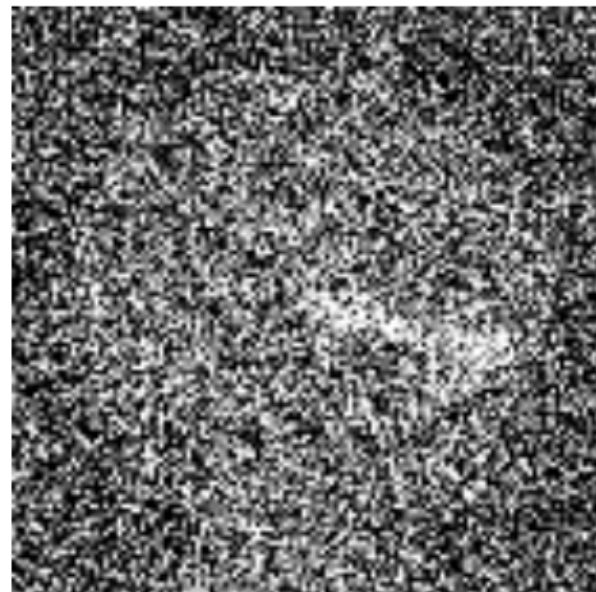
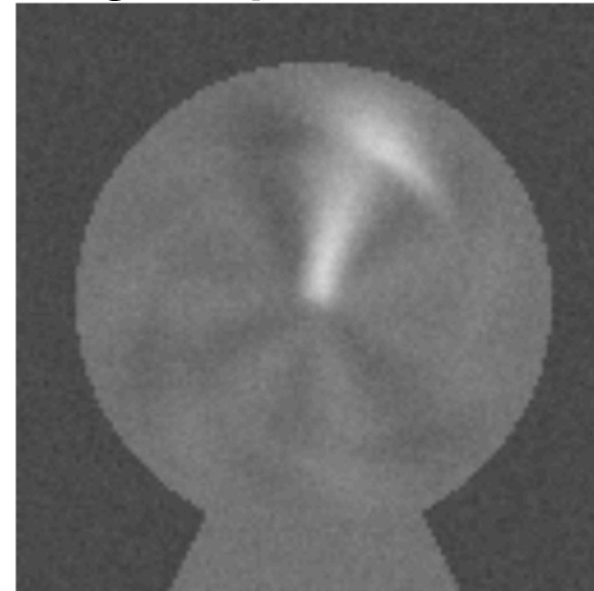
Clean clock face



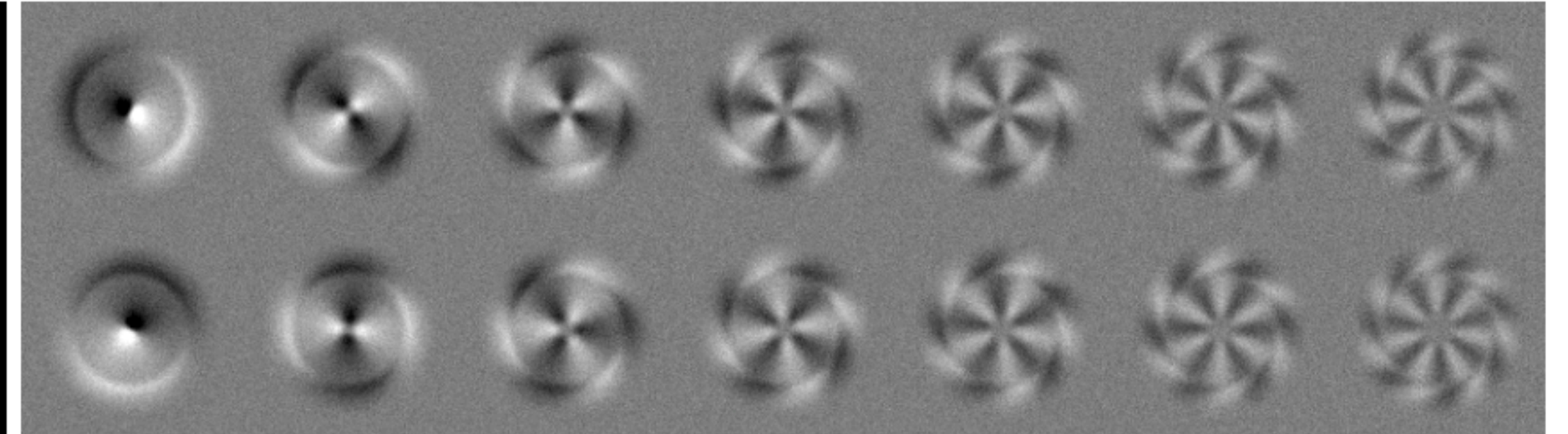
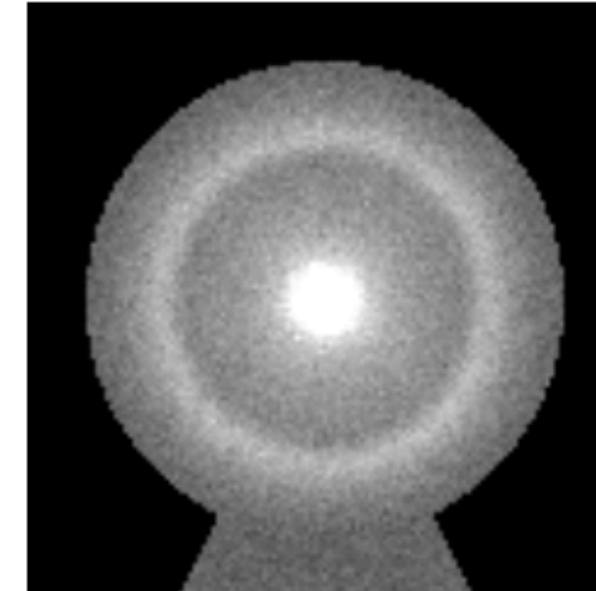
Noisy clock face



Reconstruction  
(Using 15 spectral volumes)



Spectral volumes

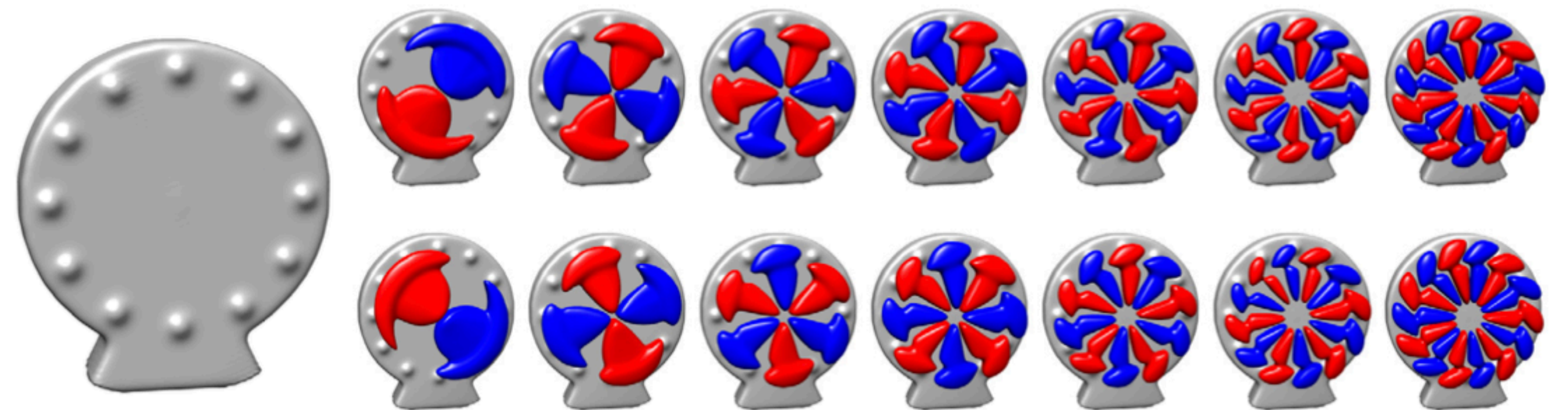


- Clock image:  $\mathbf{z}_1, \dots, \mathbf{z}_n \in \mathbb{R}^{N \times N}$
- Affinity matrix:  $W_{ij} = e^{\frac{-\|\mathbf{z}_i - \mathbf{z}_j\|^2}{N^2 \sigma^2}}$



Input model

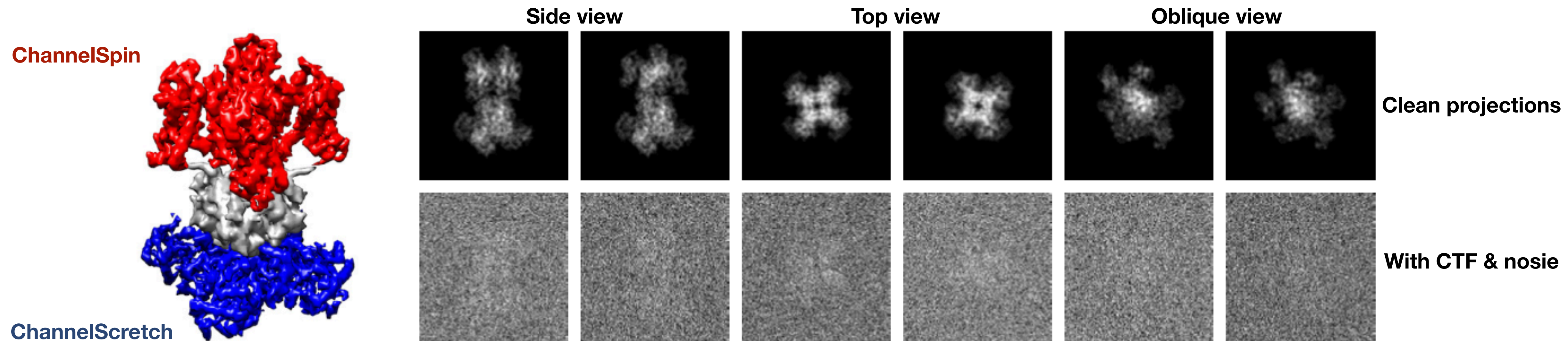
Reconstruction  
(Using 15 spectral volumes)



*Red and blue represent negative and positive values of the higher-order spectral volume, respectively.*

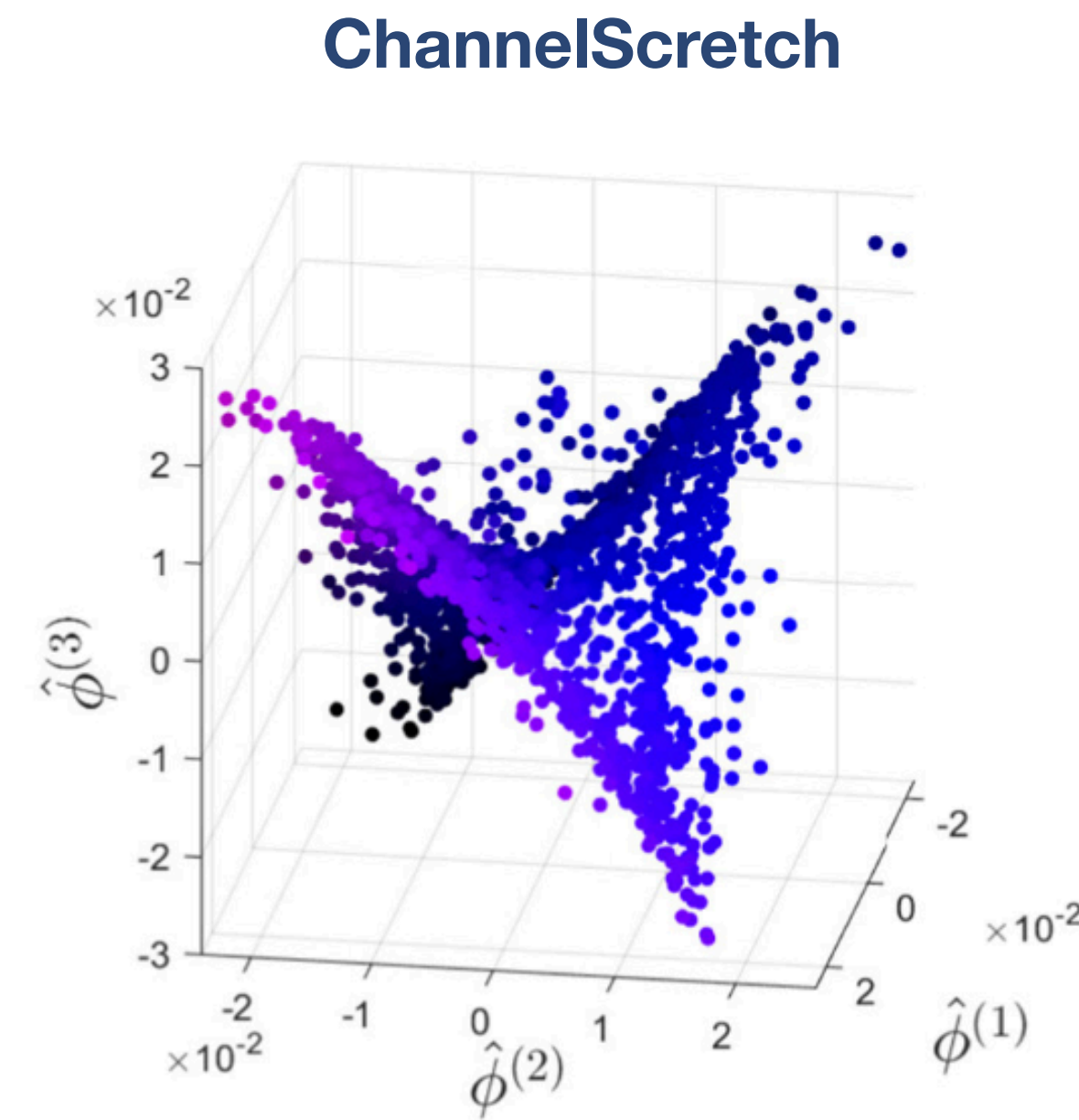
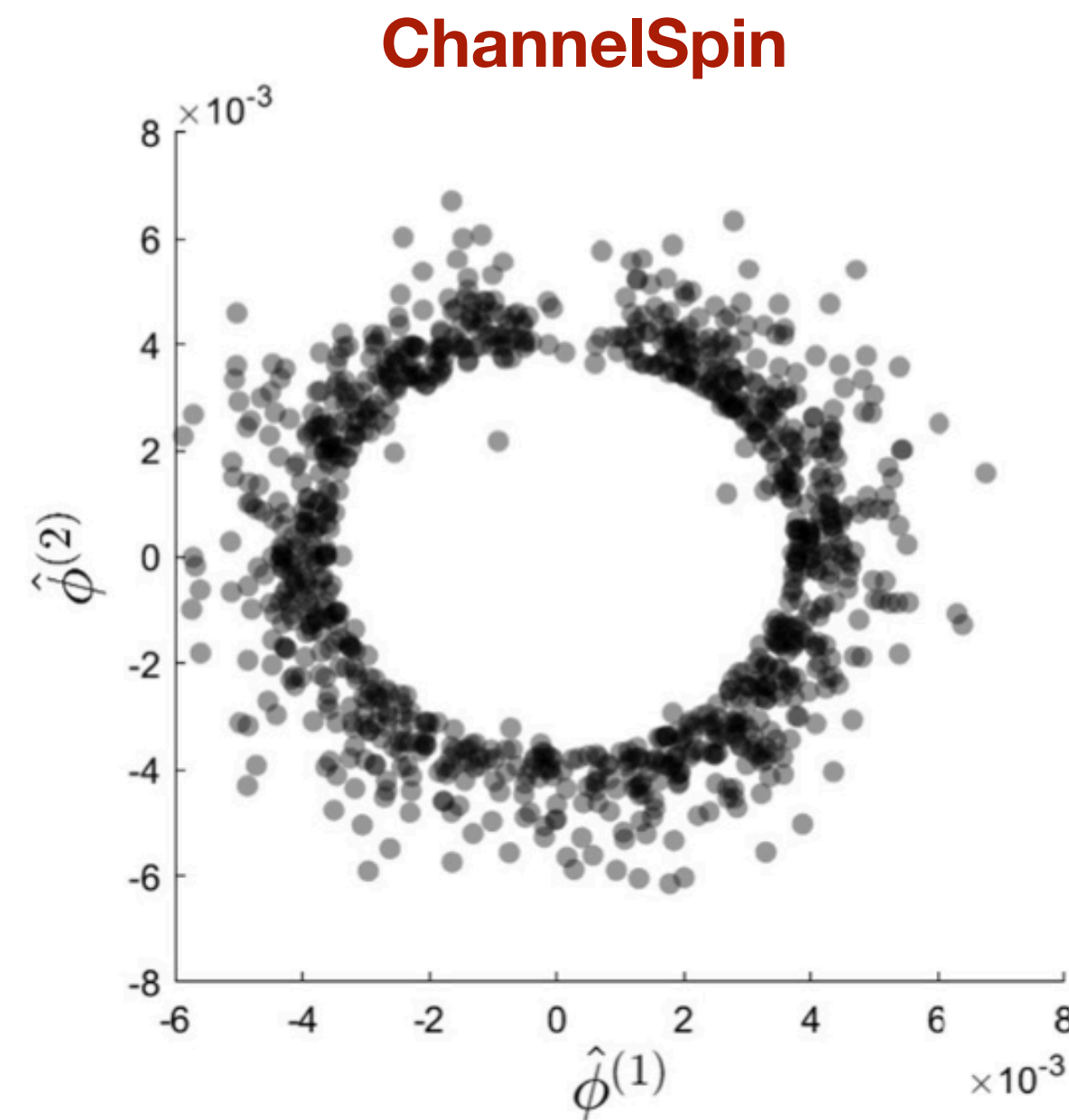


# Result — Simulated Ion Channel



- ▶ Dataset 1 — **ChannelSpin** : a rotational motion of the top part about the  $z$  axis
- ▶ Dataset 2 — **ChannelSretch** : a nonrigid stretching of the bottom part along the  $x - y$  plane
- Test conditions:
  - ▶ Total energy of the noise was 30 times that of the total energy of each clean image.
  - ▶ No in-plane shift was applied.
  - ▶ Reconstructed the volumes using  $r = 1, \dots, 15$  spectral volumes.
  - ▶ Used the true orientations of the projection images for both the covariance and spectral volume estimation procedures.
- Special resolution  $N = 108$
- #volumes  $n = 10000$  per dataset

# Examining the Laplacian Eigenmaps Embedding



- Random displacement:  $\delta_x, \delta_y \in \{-16, -15, \dots, 16\}$
- Original ion channel:  $\mathbf{v} \in \mathbb{R}^{N \times N \times N}$
- The stretched ion channel  $\mathbf{v}'$  is defined for every  $0 \leq z \leq N/2$  by:

$$\mathbf{v}'[x, y, z] = \mathbf{v}[x + \delta_x s_z, y + \delta_y s_z, z] \quad \text{where} \quad s_z = \left( \frac{N/2 - z}{N/2 - z_0} \right)^2$$

- The embedding of **ChannelSpin** clearly shows a circle.
- The embedding of the **ChannelSretch** dataset shows a 2-dimensional square in the  $\hat{\phi}_s^{(1)} - \hat{\phi}_s^{(2)}$  plane that is shaped like a saddle.
- Both of these results are in accordance with the underlying motion manifold.



# Examining the Spectral Volumes

Captures the mean over all rotations

ChannelSpin

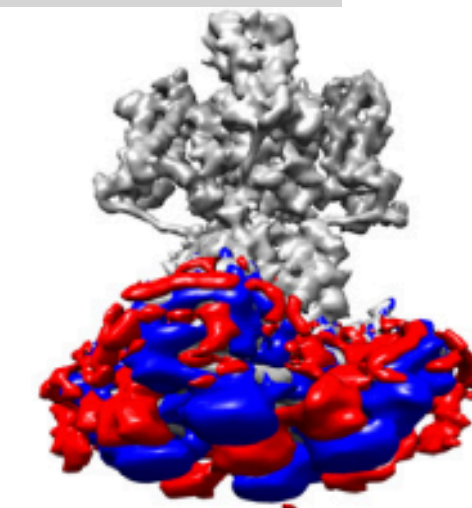
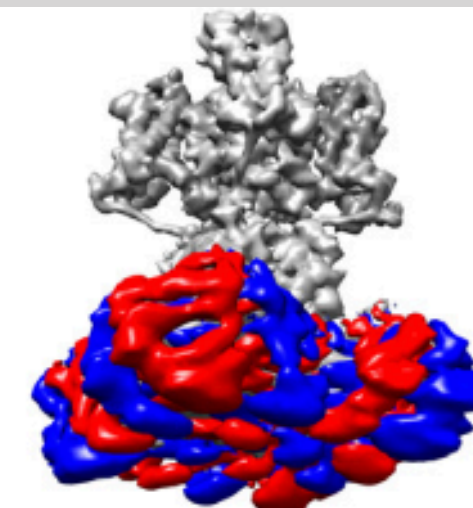
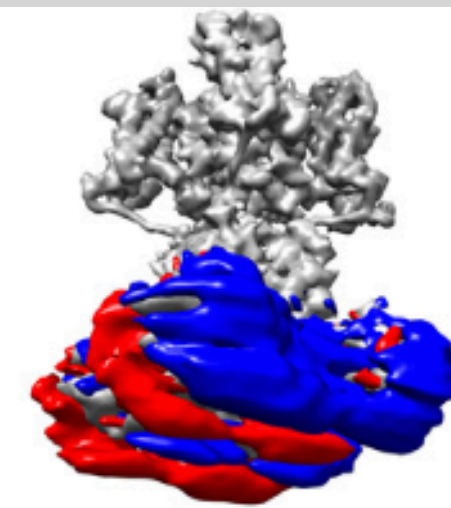
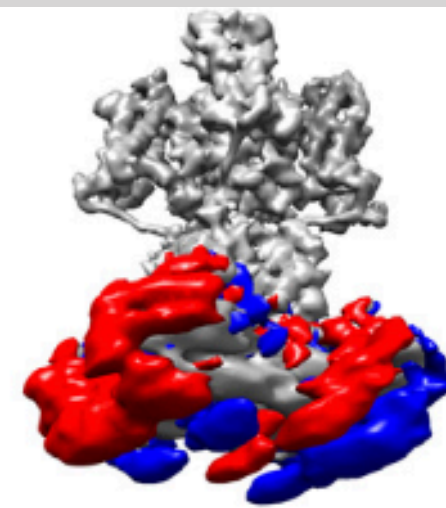
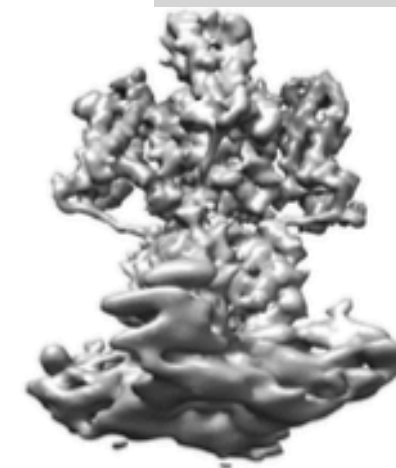


Higher order spectral volumes have increasing angular frequency, capturing more and more detail.

Due to the  $C_4$  symmetry of the ion channel, the lowest frequency has a period of 90 degrees.

Red and blue represent *negative* and *positive* values of the higher-order spectral volume, respectively.

ChannelSretch



$\hat{\alpha}^{(0)}$

$\hat{\alpha}^{(1)}$

$\hat{\alpha}^{(2)}$

$\hat{\alpha}^{(3)}$

$\hat{\alpha}^{(4)}$

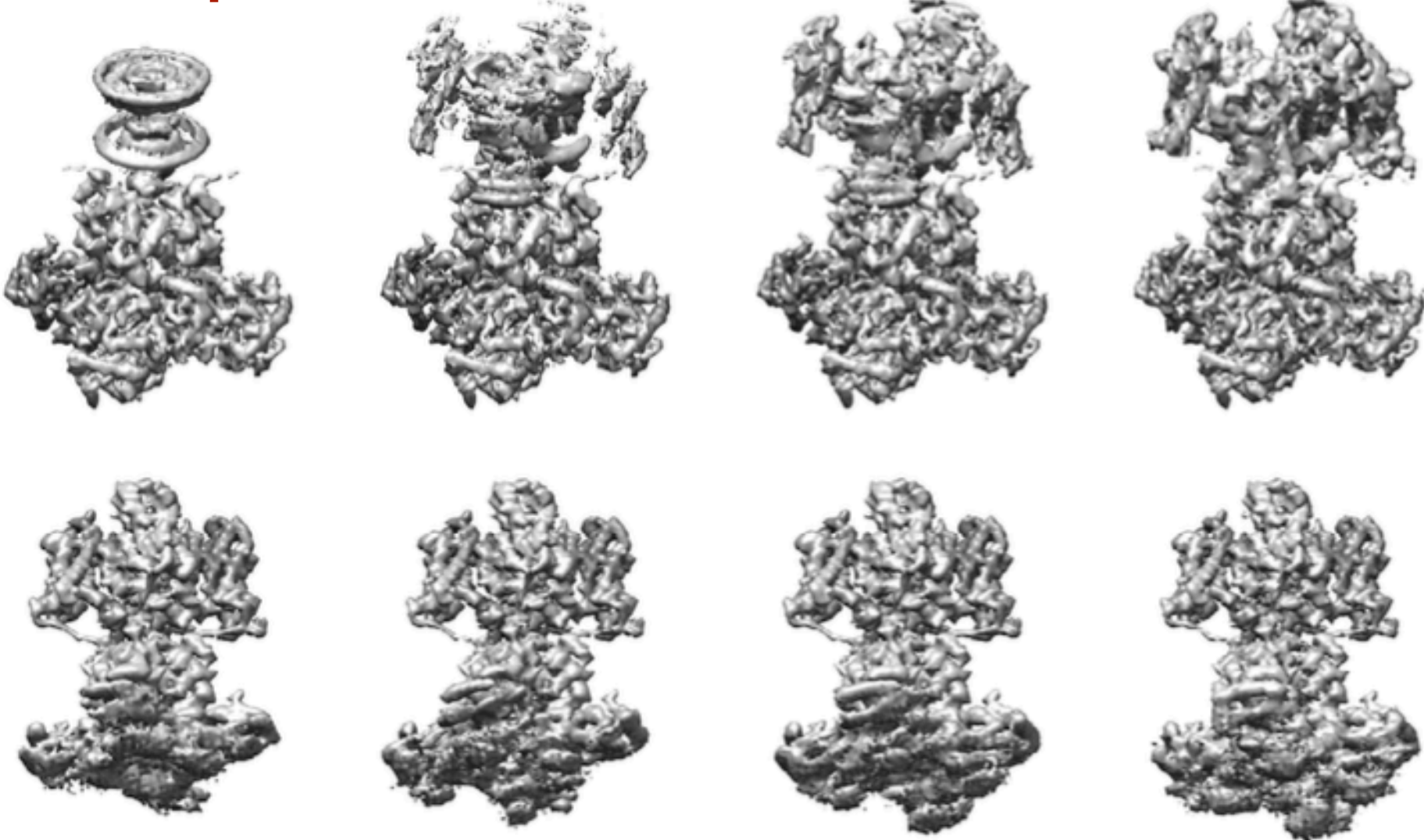
Captures the fixed part of the molecule with high resolution and shows a 'smeared' bottom portion

The first and second spectral volumes each have a low spatial frequency along the x and y axes  
Higher spectral volumes show higher spatial frequencies



# Reconstruction Accuracy and Runtime

ChannelSpin



ChannelScrech

$r = 1$        $r = 3$        $r = 5$        $r = 15$       True vol.      Cov recon.

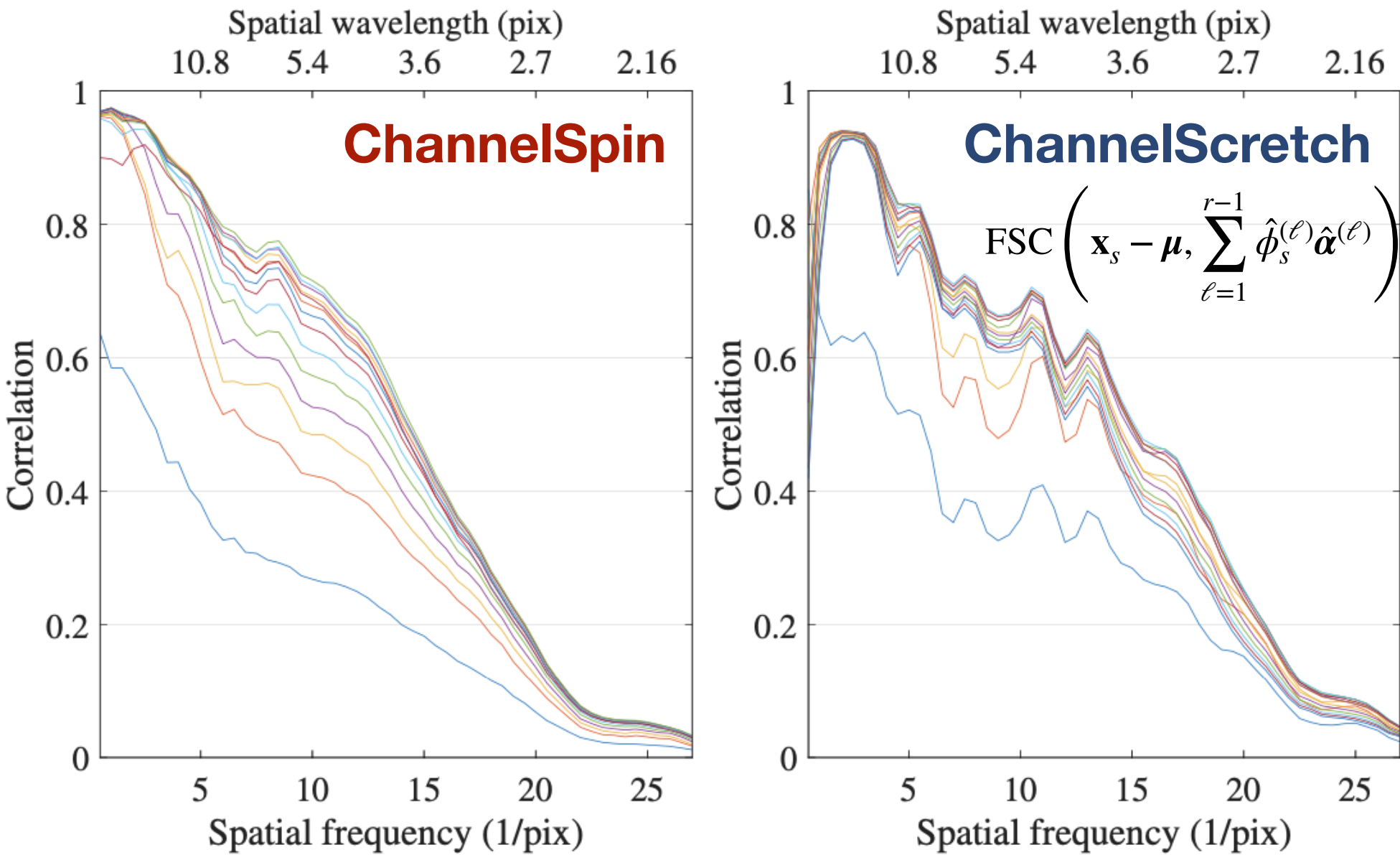


Table 2. Runtimes for the main steps of our method on the ChannelSpin dataset, with  $n = 10\,000$  images of  $108 \times 108$  pixels.

Procedure	Running time (s)
Calculation of $\hat{\boldsymbol{\mu}}$	624.6
Calculation of $\hat{\boldsymbol{\Sigma}}$	5044.7
Calculation $\hat{V}_q$	0.8
Calculation of $\{\hat{\boldsymbol{\beta}}_s\}$	2084.8
Calculation of $\{\hat{\phi}_s\}$	531.5
Calculation of $K$	12378.0
Calculation of $\mathbf{b}$	4014.1
Estimation of $\{\hat{\boldsymbol{\alpha}}^{(\ell)}\}_{\ell=0}^{15}$	1769.9

Back Up

Name	Domain	Description
$n$	$\mathbb{N}$	Number of images and underlying molecular volumes
$s$	$1, \dots, n$	Index to molecular image/volume
$N$	$\mathbb{N}$	Image/volume size
$\tilde{N}$	$\mathbb{N}$	Downsampled image/volume size
$\mathbf{x}, \mathbf{x}_s$	$\mathbb{R}^{N^3}$	Molecular volume
$\hat{\mathbf{x}}_s$	$\mathbb{R}^{N^3}$	Our high-resolution molecular volume estimate
$\mathbf{u}$	$\{1, \dots, N\}^3$	Voxel index
$\mathbf{y}, \mathbf{y}_s$	$\mathbb{R}^{N^2}$	Molecular image
$\mathbf{h}, \mathbf{h}_s$	$\mathbb{R}^{N^2}$	Contrast transfer function (CTF)
$R, R_s$	$\text{SO}(3)$	3D viewing orientation
$P, P_s$	$\mathbb{R}^{N^2 \times N^3}$	Imaging matrix (rotation, projection, and CTF)
$\mathcal{F}_d$		The $d$ -dimensional discrete Fourier transform (DFT)
$M_N$	$\mathbb{R}^N$	Sampling grid in $[-1, +1)$ used to define the DFT
$\mu$	$\mathbb{R}^{N^3}$ or $\mathbb{R}^{\tilde{N}^3}$	Mean volume (high-res or low-res)
$\Sigma$	$\mathbb{R}^{\tilde{N}^3 \times \tilde{N}^3}$	Covariance matrix of downsampled molecular volumes
$q$	$\mathbb{N}$	Number of PCA eigenvolumes
$\hat{V}_q$	$\mathbb{R}^{\tilde{N}^3 \times q}$	Eigenvolumes of the estimated covariance matrix
$\beta(\mathbf{x}), \beta_s$	$\mathbb{R}^q$	PCA coordinates of a molecular volume
$\mathbf{B}$	$\subseteq \mathbb{R}^q$	The domain of PCA coordinates
$\nu(\mathbf{B})$		Measure of volumes in PCA coordinate representation
$\mathbf{W}$	$\mathbb{R}^{n \times n}$	Edge weights matrix
$L$	$\mathbb{R}^{n \times n}$	Graph Laplacian matrix
$\mathcal{M}$	$\subset \mathbb{R}^{N^3}$	Riemannian submanifold of molecular volumes
$\phi^{(\ell)}$	$\mathbf{B} \rightarrow \mathbb{R}$	Laplace–Beltrami eigenfunction of the $\ell$ th smallest eigenvalue
$\hat{\phi}^{(\ell)}$	$\mathbb{R}^n$	Laplacian eigenvector of the $\ell$ th smallest eigenvalue
$r$	$\mathbb{N}$	Number of spectral volumes
$K$	$\mathbb{R}^{rN^3 \times rN^3}$	Matrix of weighted projection-backprojections
$\mathbf{b}$	$\mathbb{R}^{rN^3}$	Concatenation of weighted back-projection images
$\alpha^{(\ell)}$	$\mathbb{R}^{N^3}$	Spectral volumes