

Examples of FIR Filter Design with the Window Method

Dr John O' Toole

Irish Centre for Fetal and Neonatal Translational Research (INFANT)
Department of Paediatrics and Child Health,
University College Cork.
jotoole@ucc.ie
Tel: 021-4205599

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lecture notes and example questions:
https://github.com/otoolej/DSP_notes_FIR

Review: window method for FIR filter design

- procedure for window method:
 1. derive ideal impulse response $h_d[n]$ from frequency response $H_d(\omega)$
 2. select window type $w[n]$ and window length M according to design specifications
 3. shift and apply window: $h[n] = h_d[n - \frac{M-1}{2}] w[n]$
 4. filter: $y[n] = \sum_{k=0}^{M-1} h[k] x[n - k]$
- frequency-domain characteristics of window:
 - width of main lobe determines the width of filter's transition band
 - sidelobes effect ripple in pass-band and stop-bands

Learning Objectives

- different windows for designing FIR filters
- can design filter to given specifications by adjusting:
 - window type and length (M)
- more control is possible for windows with adjustable parameters (e.g. Kaiser window)
- process of designing filter given specifications.

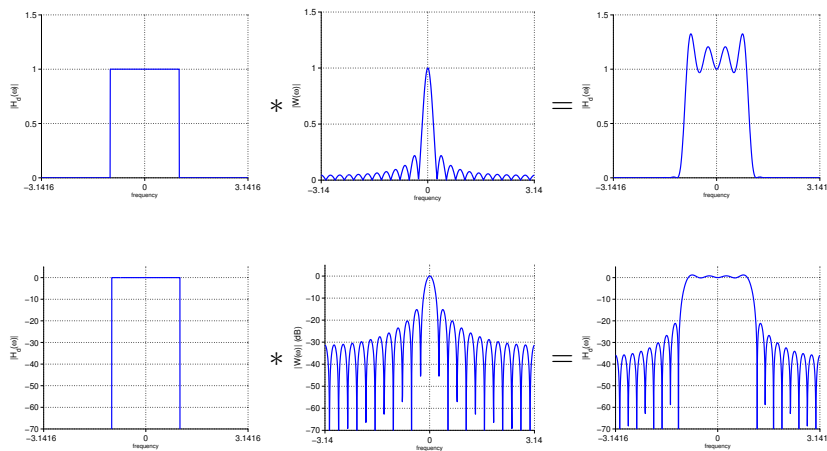
Effect of Window on Frequency Response of Filter

- why include window?
 - want $h[n]$ to be finite;
 - recall $h[n] = h_d[n - \frac{M-1}{2}] w[n]$
- consequence of limiting $h_d[n]$ in the time domain:
 - filter $y[n] = x[n] * h[n] \leftrightarrow Y(\omega) = X(\omega)H(\omega)$
 - but $h[n] = \bar{h}_d[n]w[n]$, and thus

$$y[n] = x[n] * (\bar{h}_d[n]w[n]) \leftrightarrow Y(\omega) = X(\omega) [\bar{H}_d(\omega) * W(\omega)]$$

$$(\text{with } \bar{h}_d[n] = h_d[n - (M-1)/2])$$

$$H_d(\omega) * W(\omega) = H(\omega)$$



Many different types of window functions, but

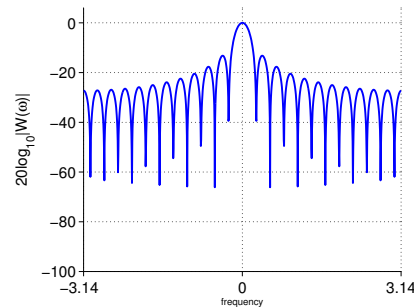
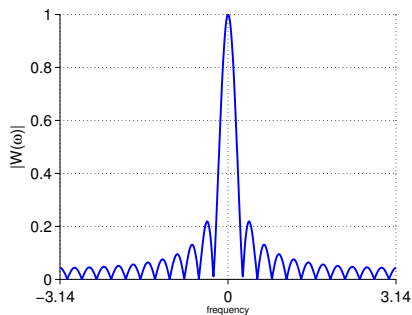
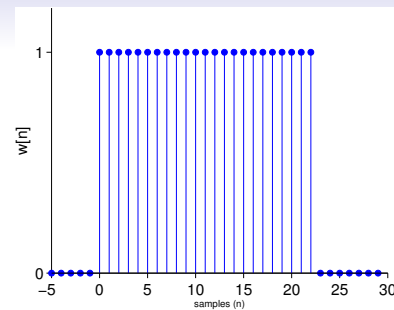
- window type determines main lobe and side lobes
- and M determines width of main lobe, **only**

effect on frequency response $H(\omega)$:

- main lobe of window \Rightarrow transition bandwidth
 - increase in M (window length) results in a decrease in the transition band
- side lobe of window \Rightarrow passband ripple and stopband attenuation
 - different window types have different levels of passband ripple

rectangular window

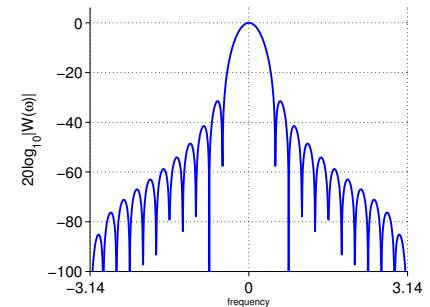
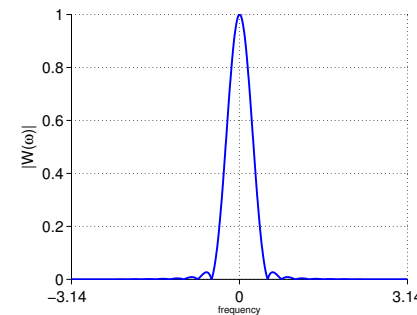
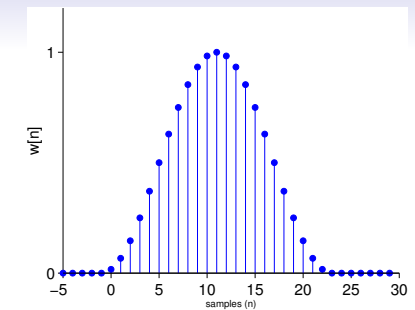
$$w[n] = \begin{cases} 1 & 0 \leq n \leq M-1 \\ 0 & \text{otherwise} \end{cases}$$



Hann (Hanning) window

$$w[n] = 0.5 - 0.5 \cos\left(\frac{2\pi n}{M-1}\right)$$

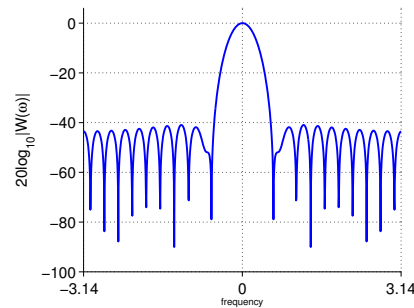
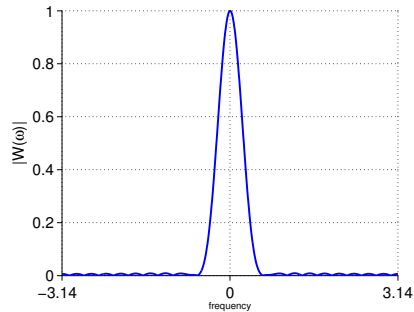
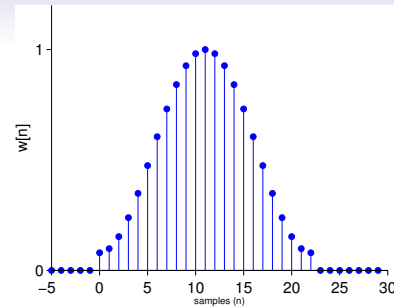
for $0 \leq n \leq M-1$ ($w[n] = 0$ otherwise).



Hamming window

$$w[n] = 0.54 - 0.46 \cos\left(\frac{2\pi n}{M-1}\right)$$

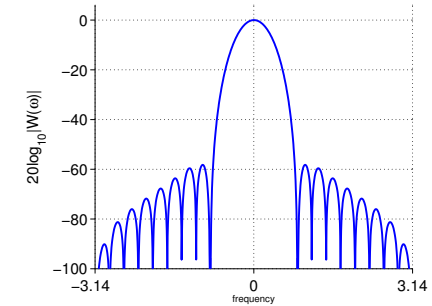
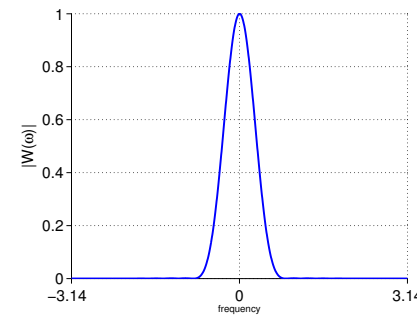
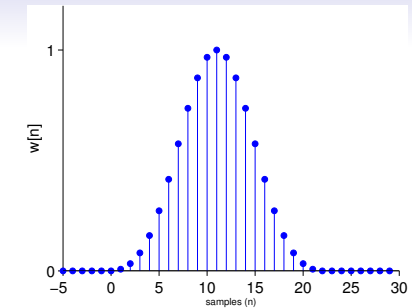
for $0 \leq n \leq M-1$ ($w[n] = 0$ otherwise).



Blackman window

$$w[n] = 0.42 - 0.5 \cos\left(\frac{2\pi n}{M-1}\right) + 0.08 \cos\left(\frac{4\pi n}{M-1}\right)$$

for $0 \leq n \leq M-1$ ($w[n] = 0$ otherwise).



Windows

- Several window functions have been proposed which lead to filters with varying transition band widths and stopband attenuation for a **fixed filter length**.
- Can relate the transition band width ($\Delta\omega$) to the filter length. For example the Blackman Window $\Delta\omega \approx -12\pi/M$.
- Can determine approximately the minimum stopband attenuation that can be achieved with a particular window. For example with the Hanning Window it is **44 dB**.
- Can determine approximately the passband ripple. For example with the Hamming Window it is **0.0194 dB**.

Window Specifications

window type	side-lobe amplitude (dB)	Approx. width of main lobe ($\approx \Delta\omega$)	Approx. stopband $20 \log_{10}(\delta)$ (dB)	Approx. passband $20 \log_{10}(1 + \delta)$ (dB)
rectangular	-13	$4\pi/(M+1)$	-21	0.7416
Hanning	-31	$8\pi/M$	-44	0.0546
Hamming	-41	$8\pi/M$	-53	0.0194
Blackman	-57	$12\pi/M$	-74	0.0017

(Discrete-Time Signal Processing, Oppenheim *et al.*, 2nd Ed., pp. 471)

- transition width ($\Delta\omega$) for 4 windows (rectangular, Hanning, Hamming, and Blackman windows) \approx main lobe of window
- passband and stopband ripple are equal $\delta = \delta_1 = \delta_2$

Kaiser Window

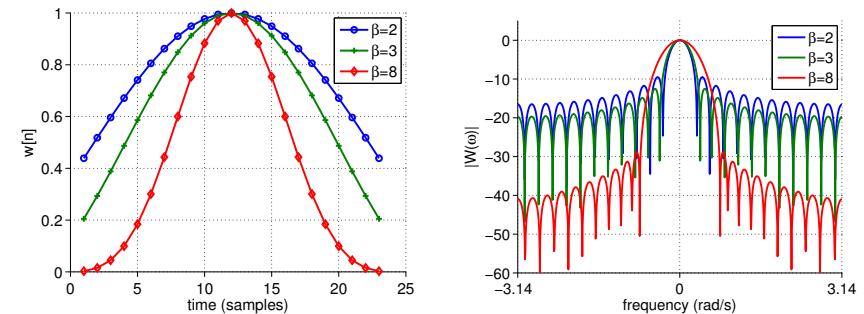
window function with parameter β to control shape of the window:

$$w[n] = \begin{cases} \frac{I_0[\beta(1-[(n-M_h)/M_h]^2)]^{1/2}}{I_0(\beta)} & 0 \leq n \leq M-1 \\ 0 & \text{otherwise} \end{cases}$$

where $M_h = (M-1)/2$, I_0 is zero-order modified Bessel function of the first kind.

- two parameters M and β control *both* main lobe width and side lobe amplitude
- \Rightarrow more precise than selecting a window (e.g. Hamming) which has set side lobe amplitude;

Kaiser window with $M = 23$



Parameter β controls both main and side lobes.

Filter Design with Kaiser Window

- given filter specifications: transition width $\Delta\omega$ and pass-band ripple δ_1 (or minimum stopband attenuation δ_2 , with $\delta = \delta_1 = \delta_2$), then find M and β
- first let $A = -20 \log_{10} \delta_p$, then

$$\beta = \begin{cases} 0.1102(A - 8.7) & A > 50 \\ 0.5842(A - 21)^{0.4} + 0.07886(A - 21) & 21 \leq A \leq 50 \\ 0 & A < 21 \end{cases}$$

- and

$$M = \frac{A - 8}{2.285\Delta\omega}$$

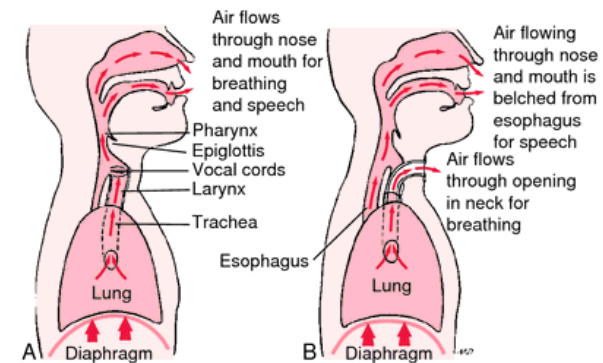
Comparison of Windows

window type	peak side-lobe amplitude (dB)	Approx. width of main lobe ($\approx \Delta\omega$)	Approx. stopband $20 \log_{10}(\delta)$ (dB)	Kaiser parameter β	Transition width of Kaiser $\Delta\omega$
rectangular	-13	$4\pi/(M+1)$	-21	0	$1.81\pi/M$
Hanning	-31	$8\pi/M$	-44	3.86	$5.01\pi/M$
Hamming	-41	$8\pi/M$	-53	4.86	$6.27\pi/M$
Blackman	-57	$12\pi/M$	-74	7.04	$9.19\pi/M$

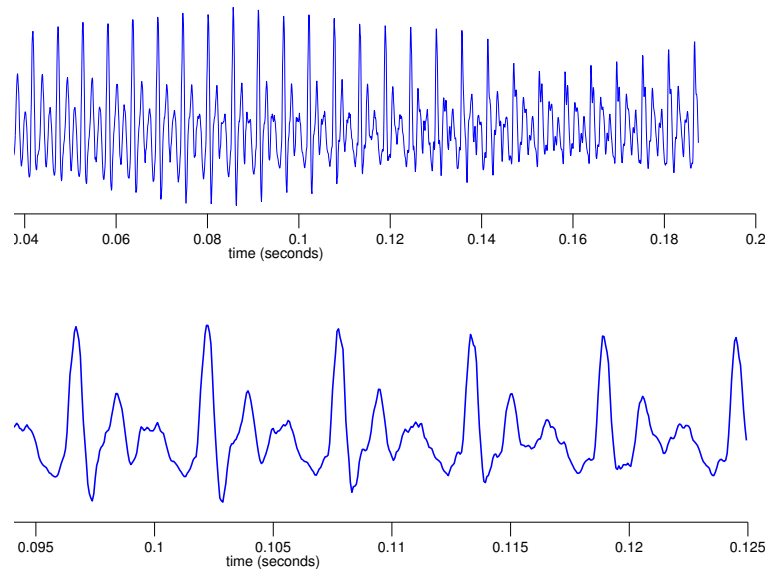
Filter Design Example: Enhancing Oesophageal Speech

- cancer of the larynx accounts for 3% of all cancers
 - main risk factors: male, alcohol, and smoking;
- treatment includes removal of larynx:
 - no vocal-folds: how to speak? (vocal-folds vibrate to produce glottal waveform)
- possible modes of speech:
 - electro-larynx
 - insert prosthetic device between trachea and oesophagus (trache-oesophageal puncture)
 - oesophageal phonation

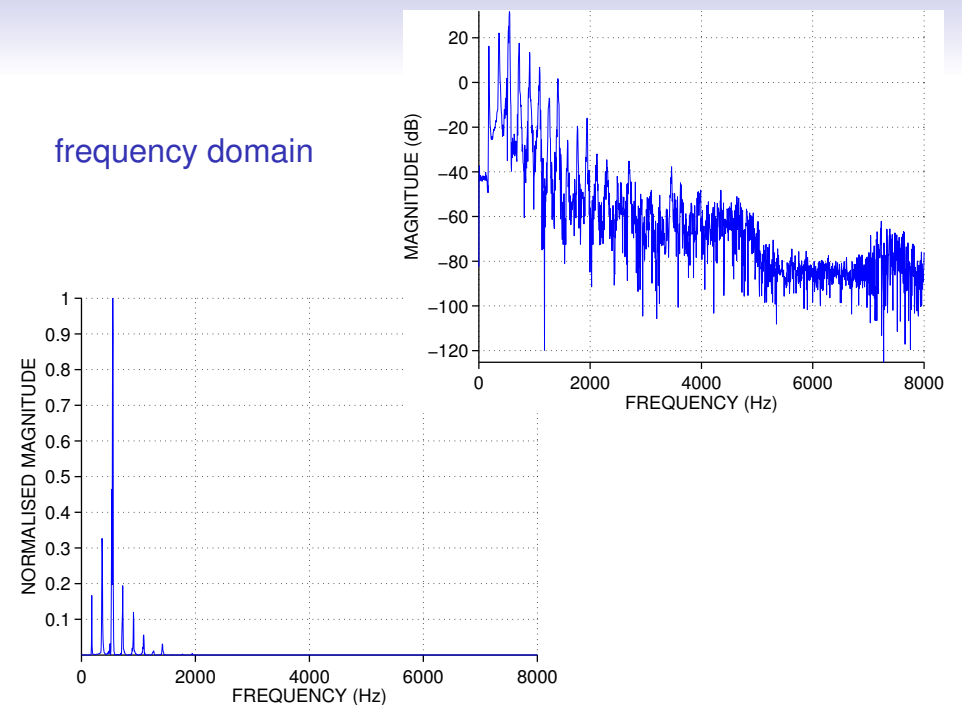
- oesophageal speech:
 - suck air down through the oesophagus, then expel to mimic glottal waveform
- problems with oesophageal speech: intelligibility and quality
- possible solution: signal processing to enhance speech



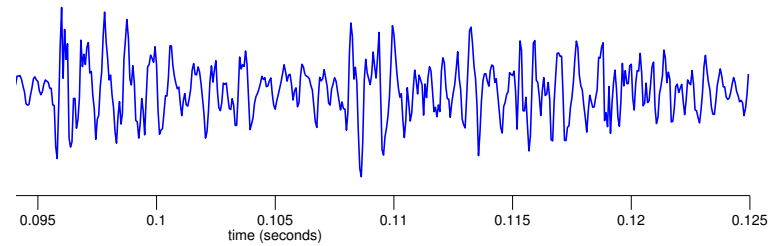
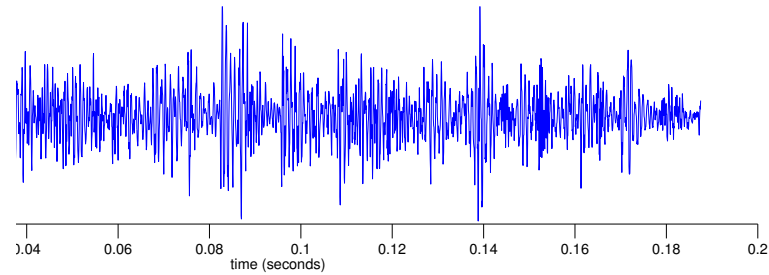
example of voiced speech (time-domain)



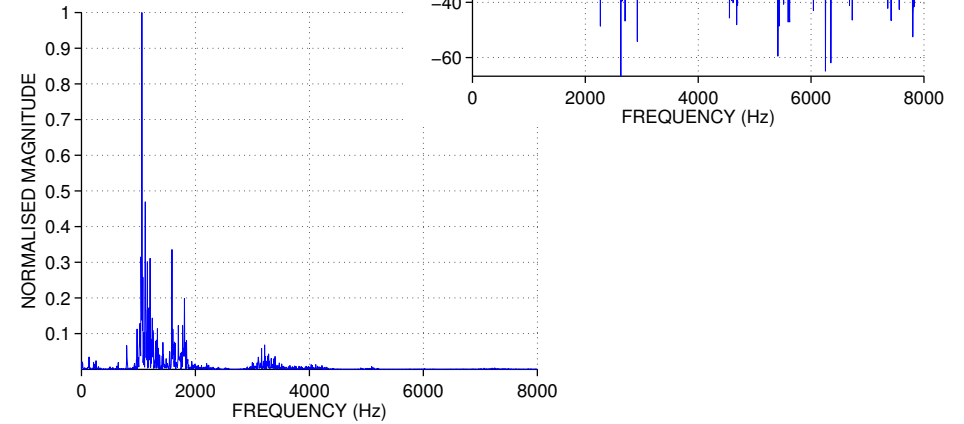
frequency domain



example of oesophageal (voiced) speech



frequency domain



Design low-pass FIR filter

find impulse response $h[n]$ coefficients if:

- pass-band edge frequency: $f_p = 2.5$ kHz
- transition width 200 Hz
- sampling frequency 16 kHz

select: M (filter length) and window type $w[n]$.

ideal low pass filter:

$$H_d(\omega) = \begin{cases} 1 & 0 \leq |\omega| \leq \omega_c \\ 0 & \text{otherwise} \end{cases}$$

inverse DTFT:

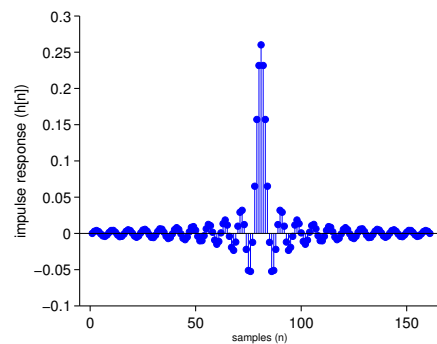
$$\begin{aligned} h_d[n] &= \frac{1}{2\pi} \int_{-\pi}^{\pi} H_d(\omega) e^{j\omega n} d\omega \\ &= \frac{1}{2\pi} \int_{-\omega_c}^{\omega_c} e^{j\omega n} d\omega \\ &= \begin{cases} \frac{\sin(\omega_c n)}{\pi n} & n \neq 0 \\ \frac{\omega_c}{\pi} & n = 0 \end{cases} \end{aligned}$$

impulse response function $h[n]$

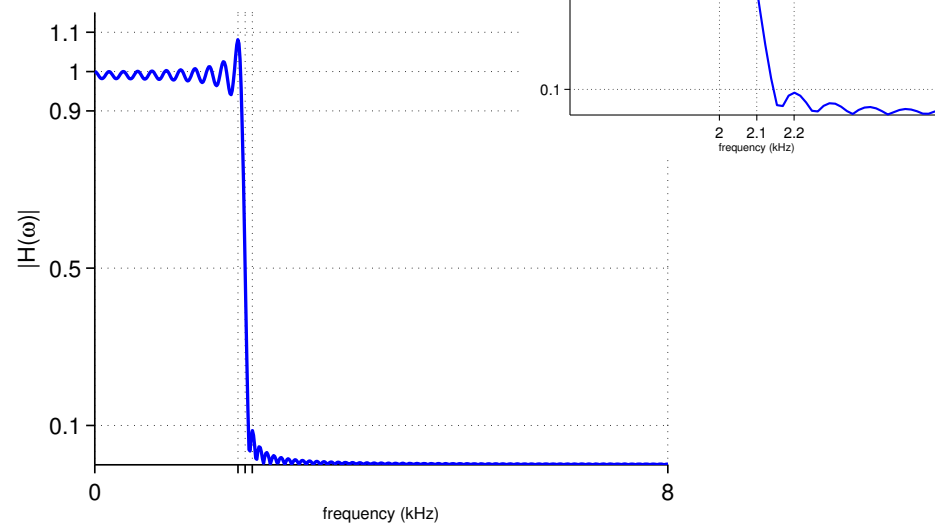
$$M = \frac{4\pi}{\Delta\omega} - 1$$

$$= \left\lceil \frac{4\pi}{(200/16000)(2\pi)} \right\rceil_{\text{odd}}$$

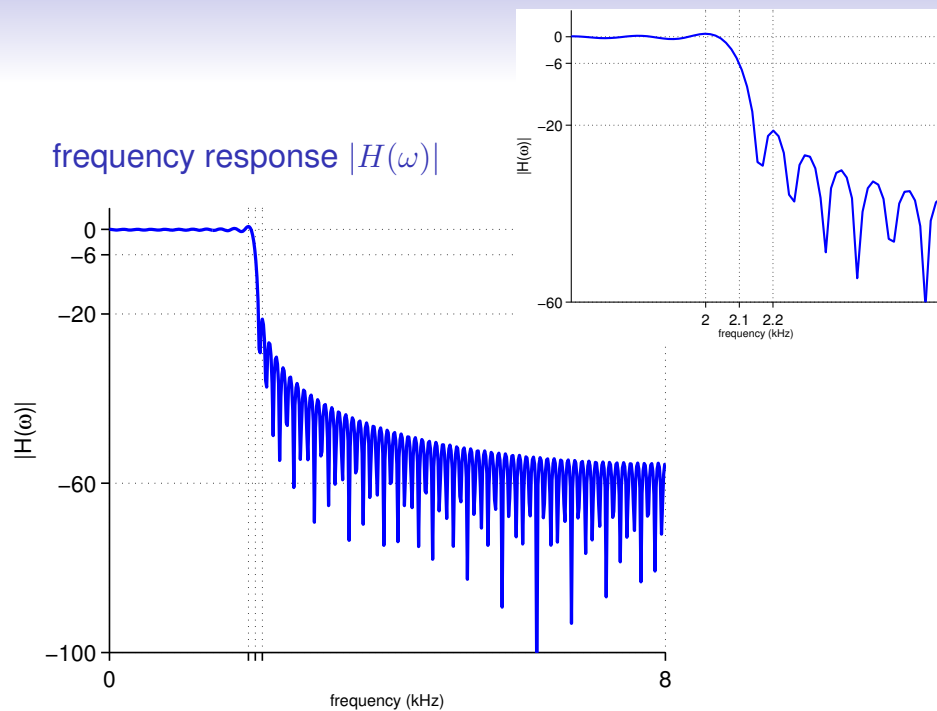
$$= 159$$



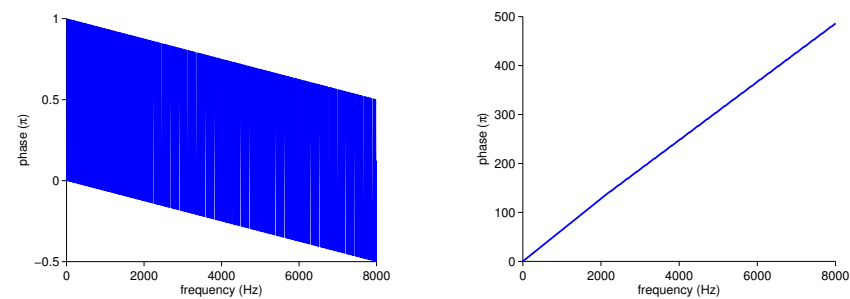
frequency response $|H(\omega)|$



frequency response $|H(\omega)|$

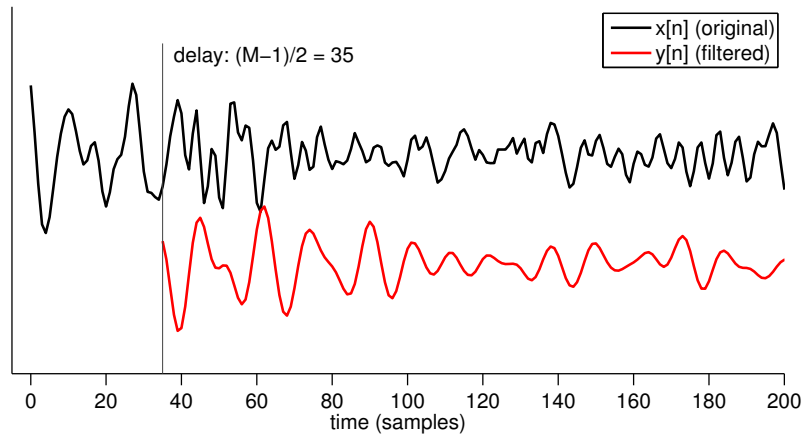


phase $\theta(\omega)$ ($M = 71$)

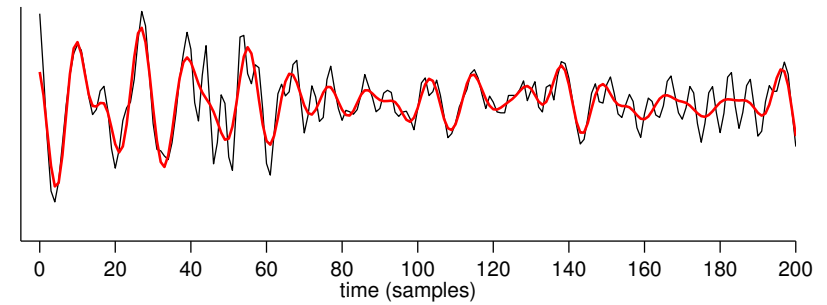


use impulse response $h[n]$ to filter oesophageal speech signal $x[n]$ ($M = 71$):

$$y[n] = \sum_{k=0}^{70} h[k]x[n-k]$$



shift $y[n]$ to compare:

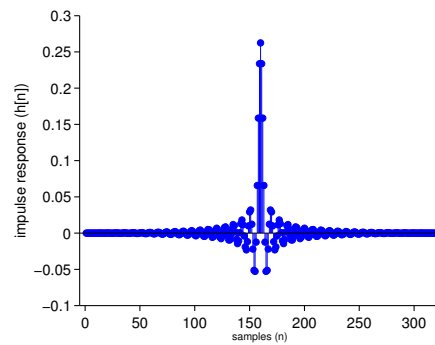


impulse function $h[n]$ with Hann (Hanning) window

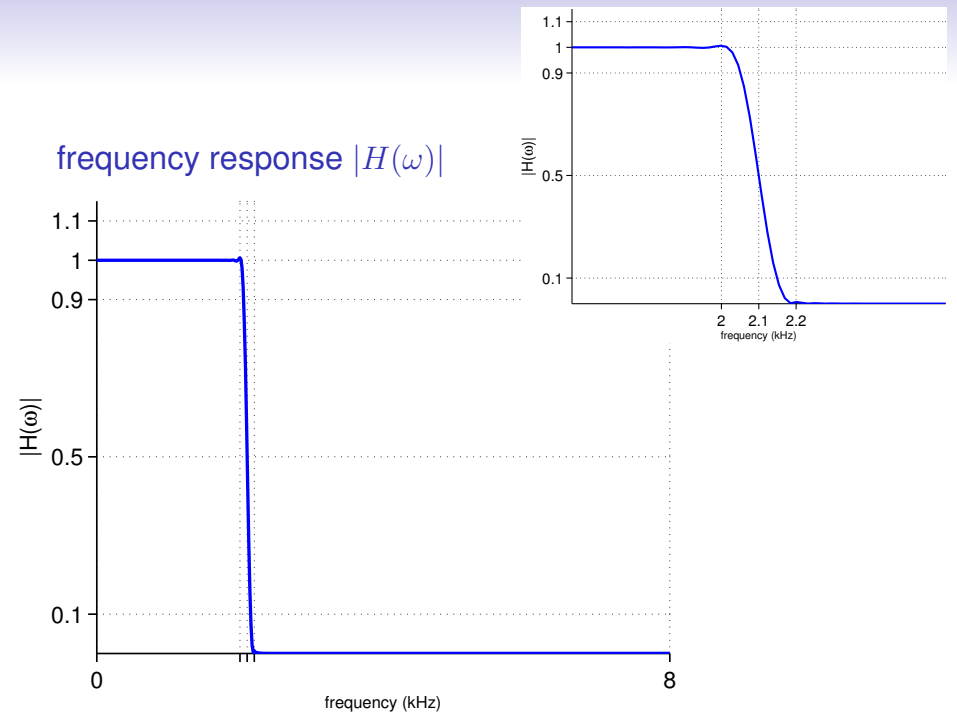
$$M = \frac{8\pi}{\Delta\omega}$$

$$= \left\lceil \frac{8\pi}{(200/16000)2\pi} \right\rceil_{\text{odd}}$$

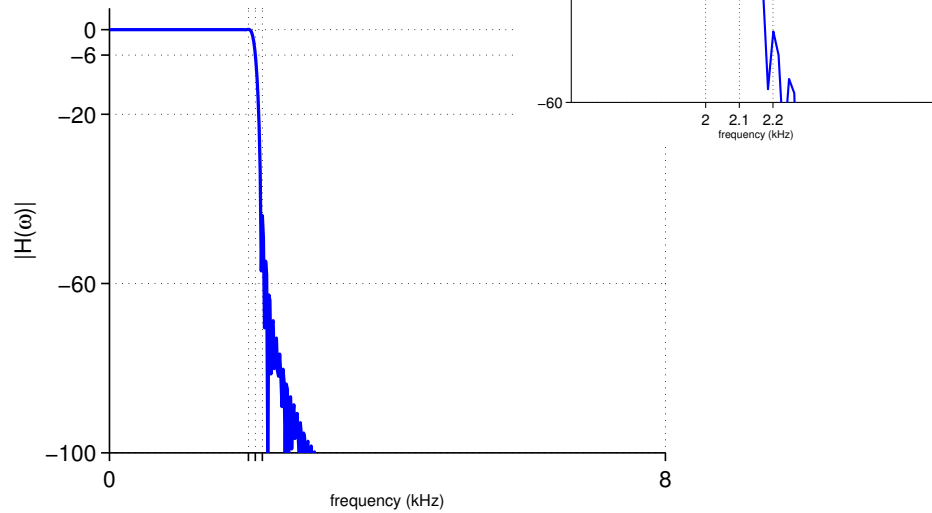
$$= 319$$



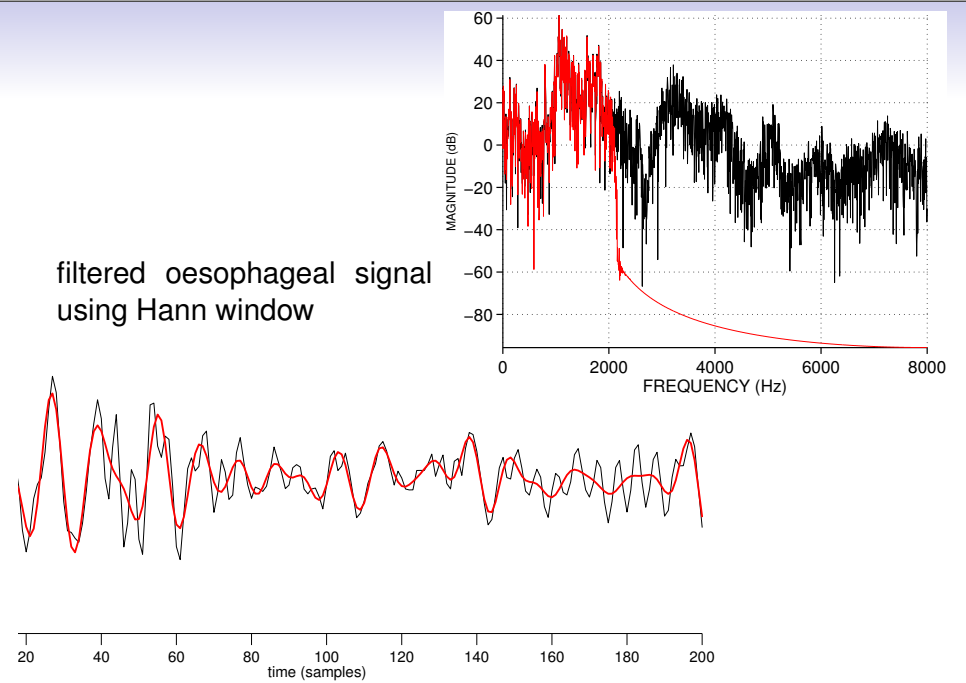
frequency response $|H(\omega)|$



frequency response $|H(\omega)|$



filtered oesophageal signal
using Hann window

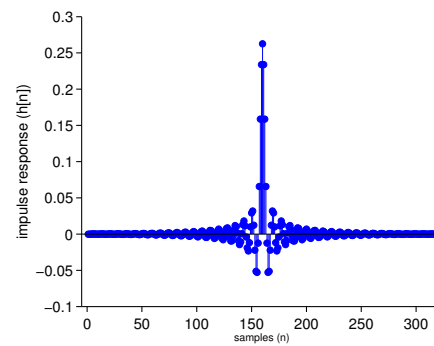


impulse function $h[n]$ with Hamming window

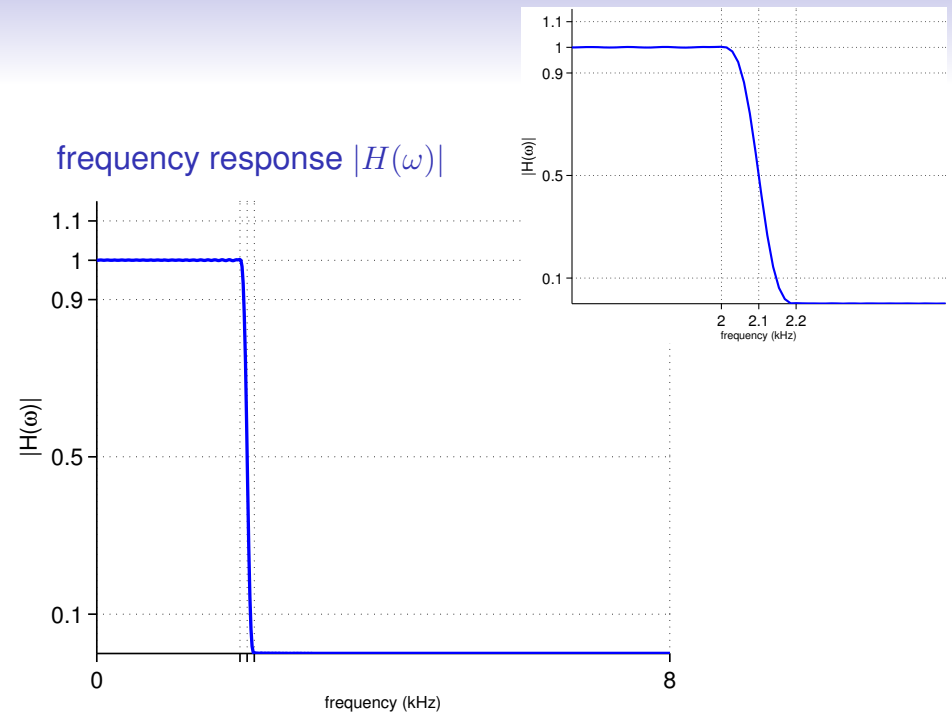
$$M = \frac{8\pi}{\Delta\omega}$$

$$= \left\lceil \frac{8\pi}{(200/16000)2\pi} \right\rceil_{\text{odd}}$$

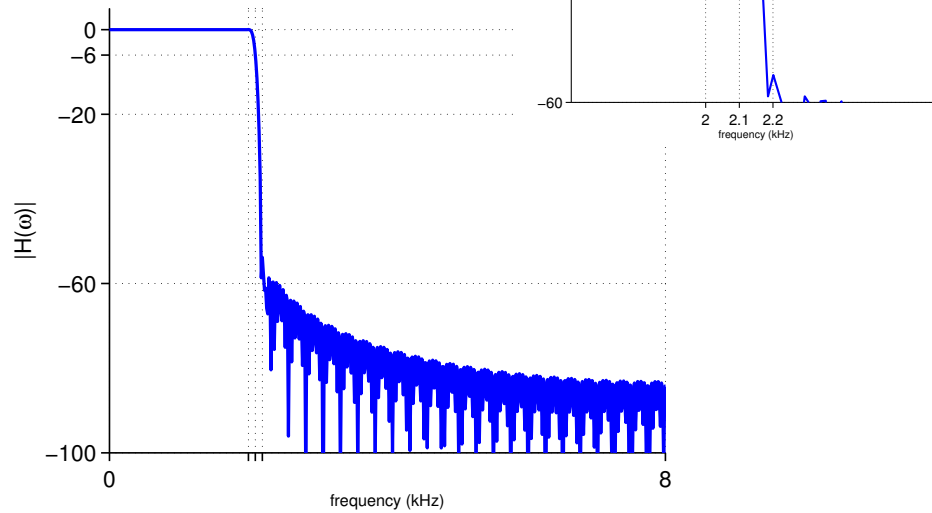
$$= 319$$



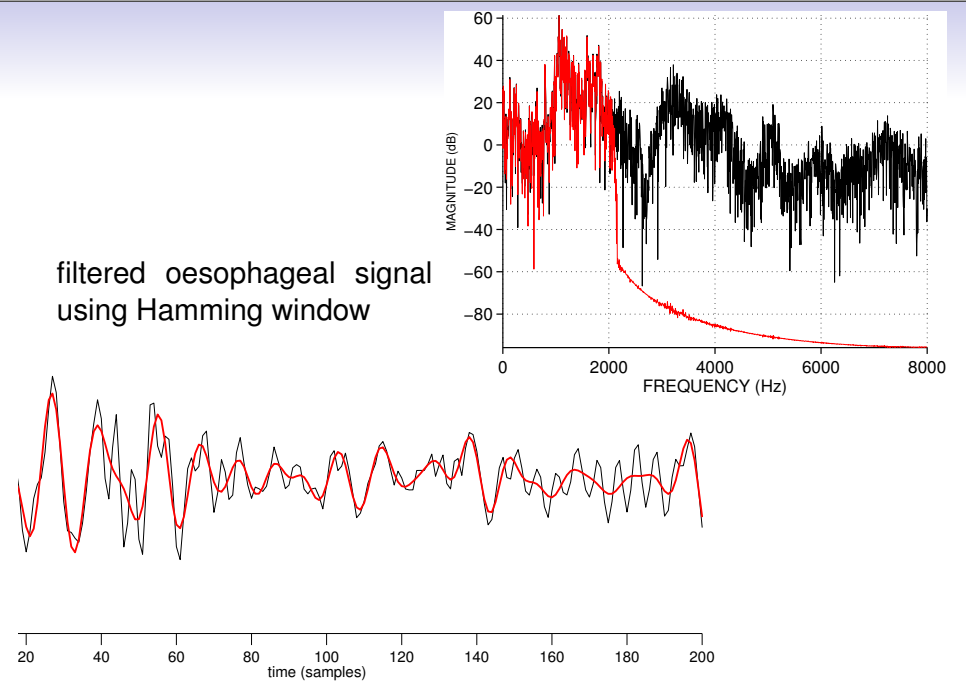
frequency response $|H(\omega)|$



frequency response $|H(\omega)|$



filtered oesophageal signal
using Hamming window

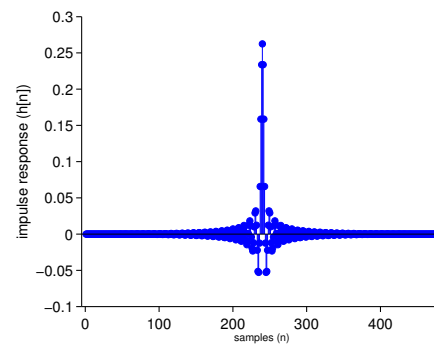


impulse function $h[n]$ with Blackman window

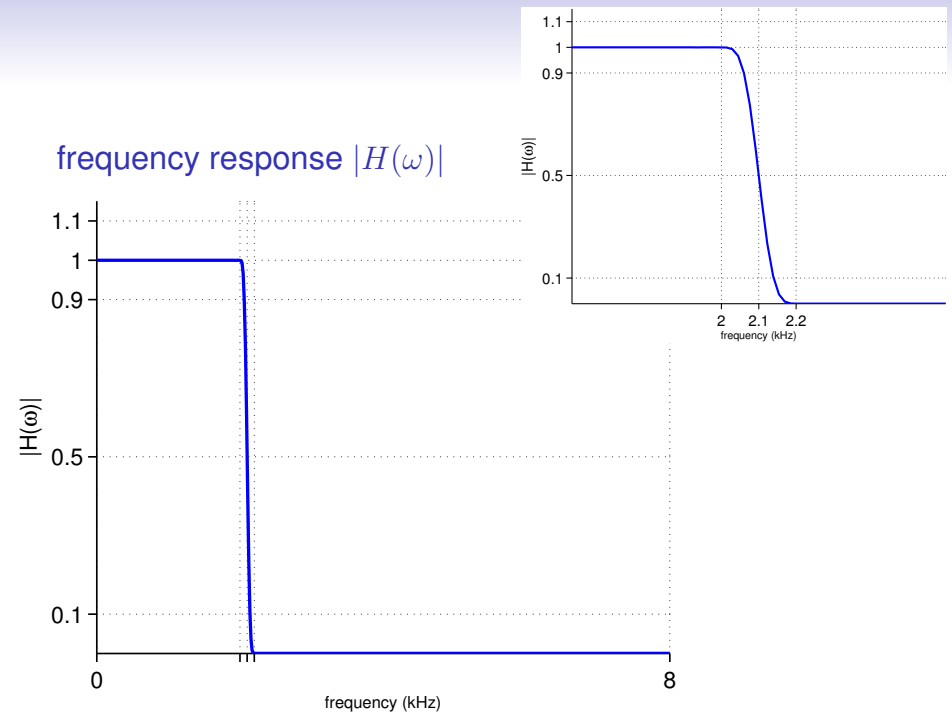
$$M = \frac{12\pi}{\Delta\omega}$$

$$= \left\lceil \frac{12\pi}{(200/16000)2\pi} \right\rceil_{\text{odd}}$$

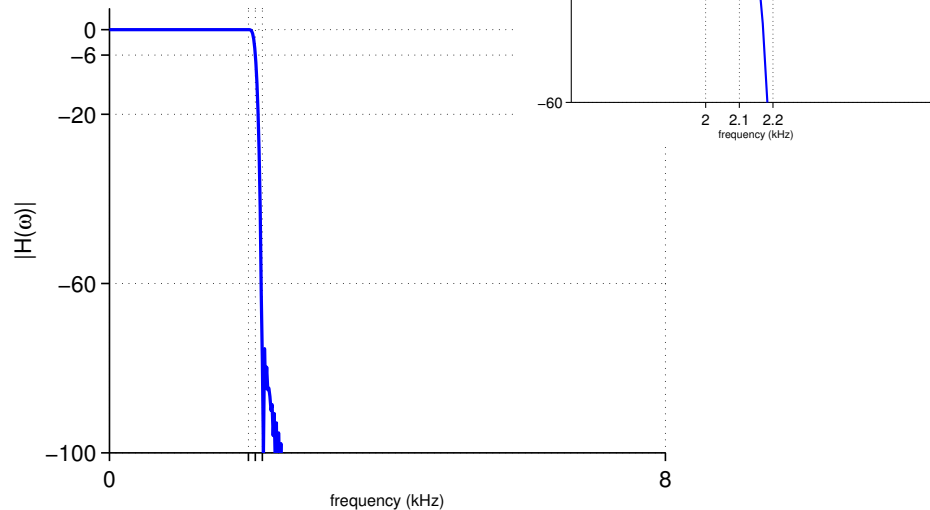
$$= 479$$



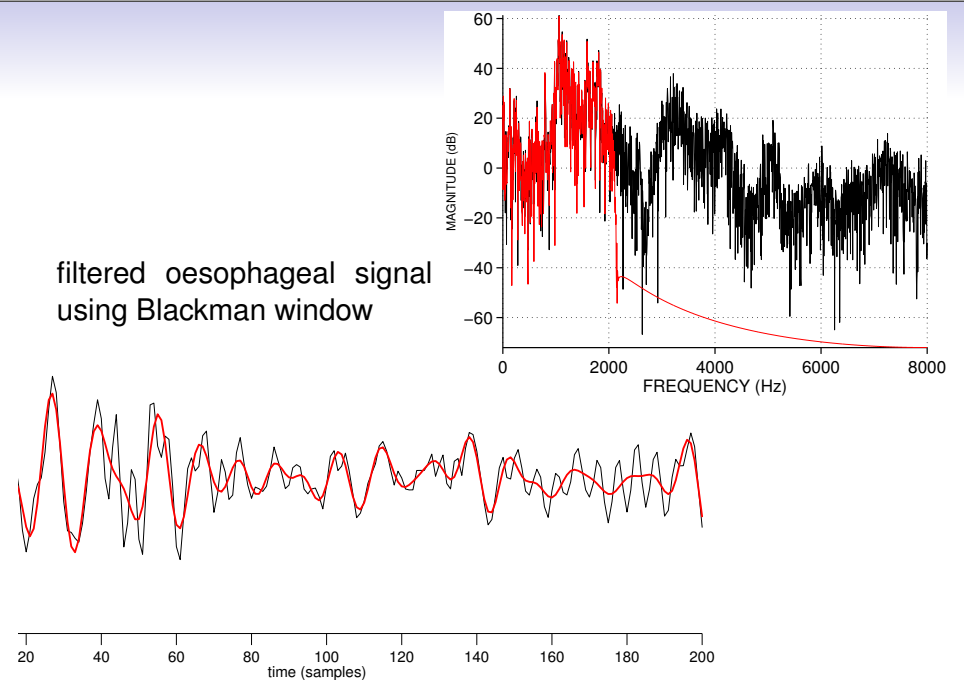
frequency response $|H(\omega)|$



frequency response $|H(\omega)|$



filtered oesophageal signal
using Blackman window



which window to use and why?

should consider:

- transition width, but can adjust M accordingly
 - increasing M increases computational load and delay, but not a problem here (max. 15 ms delay)
- stop band attenuation and pass/stop-band ripple:
 - Hann, Hamming, and Blackman seem adequate
- which one: either Hann, Hamming, and Blackman?
- what about Kaiser window?
 - if $\beta = 7.04$ for example, then min. stopband attenuation is -74 dB, which is equal to the Blackman window.
 - but, transition width differ ($12\pi/M$ vs. $9.19\pi/M$)
 - therefore, for Kaiser $M = 369$ vs. $M = 480$ for Blackman

precise design with Kaiser window:

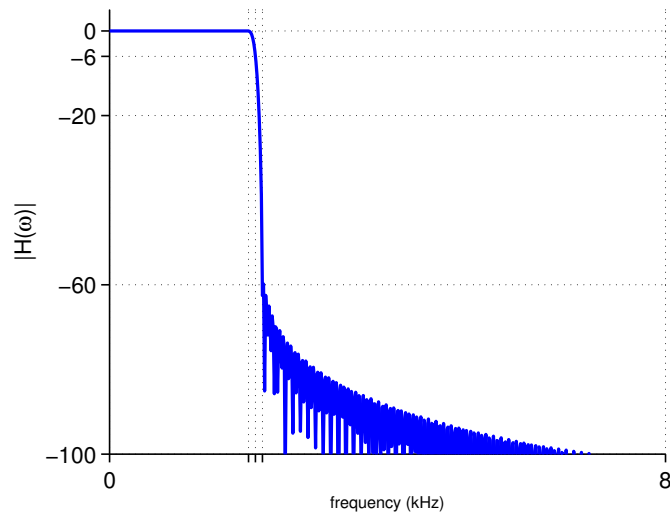
- what if we required stopband attenuation of -60 dB and $M < 300$
 - could use Blackman window (with stopband -74 dB), but $M = 479$ (see previous slides)
- solution: use Kaiser window with

$$\beta = 0.1102(A - 8.7) = 5.633$$

where $A = -20 \log_{10}(\delta) = 60$ and

$$M = \frac{A - 8}{2.285\Delta\omega} = 289.7525 = \lceil 289.7525 \rceil_{\text{odd}} = 291$$

Low-pass filter with Kaiser window ($M = 291$ and $\beta = 5.633$):



Summary: Window Method FIR Filter Design

- Pro: simplicity
- Con: lack of flexibility: peak pass-band and peak stop-band ripples are approx. equal
 - may not suit design
- Con: convolution of spectral window with ideal frequency response means that pass-band and stop-band edge frequencies are not precisely specified
- Con: may not be able to determine $h_d[n]$ from $H_d(\omega)$
- Con: for a given window, stop-band attenuation is fixed (i.e. independent of M)
 - need to find suitable window
- Kaiser window includes a parameter which allows a trade off between transition width and ripple.