## Computational MRI

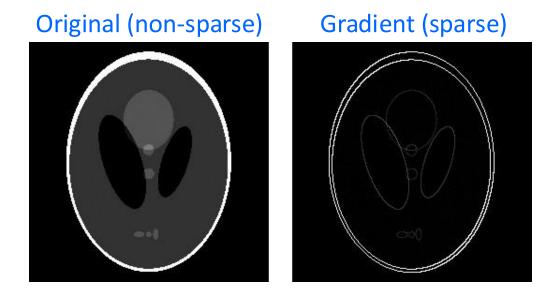
#### **Compressed Sensing**





#### Compressed sensing: The big picture

 Exploit image sparsity/compressibility to reconstruct undersampled data



Which image would require fewer samples?

- Nyquist: same FOV, same number of samples
- Common sense: fewer non-zero pixels, fewer samples

#### Image compression

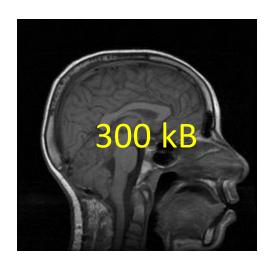




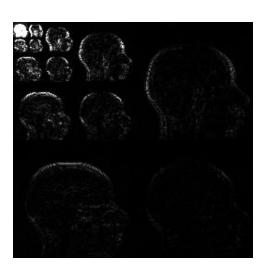


- Essential tool for modern data storage and transmission
- Exploit pixel correlations to reduce number of bits
- First reconstruct, then compress

Fully-sampled acquisition (Nyquist rate)

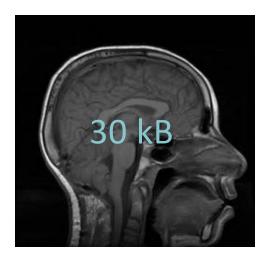


Sparsifying transform (e.g. wavelets)



Store or transmit non-zero coefficients only

Recover image from sparse coefficients



10-fold compression

#### Nyquist sampling is inefficient

#### Question

– Why do we need to acquire samples at the Nyquist rate if we are going to throw away most of them?

#### Answer

- We don't. Do compressed sensing instead
- Build data compression in the acquisition
- First compress, then reconstruct

Candès E, Romberg J, Tao T. IEEE Trans Inf Theory 2006; 52(2): 489-509

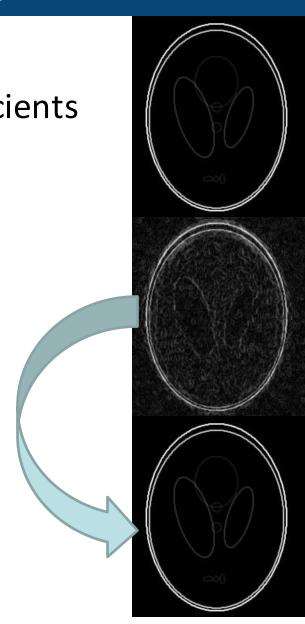
Donoho D. IEEE Trans Inf Theory 2006; 52(4): 1289-1306.



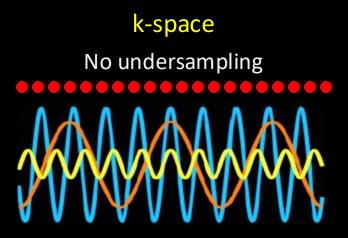


## Compressed sensing components

- Sparsity
  - Represent images with a few coefficients
  - Transform: wavelets, gradient, etc.
- Incoherence
  - Noise-like aliasing artifacts
- Non-linear reconstruction
  - Remove aliasing artifacts



#### Simple compressed sensing example



Regular undersampling

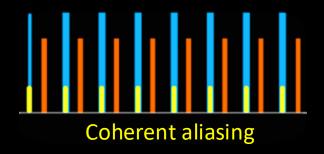
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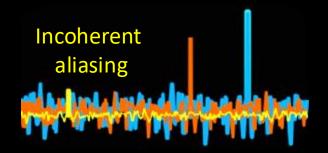
Random undersampling

0 • • 0 0 0 • 0 • 0 • 0 0 0 0 0 0 0

Image space







Courtesy of Miki Lustig

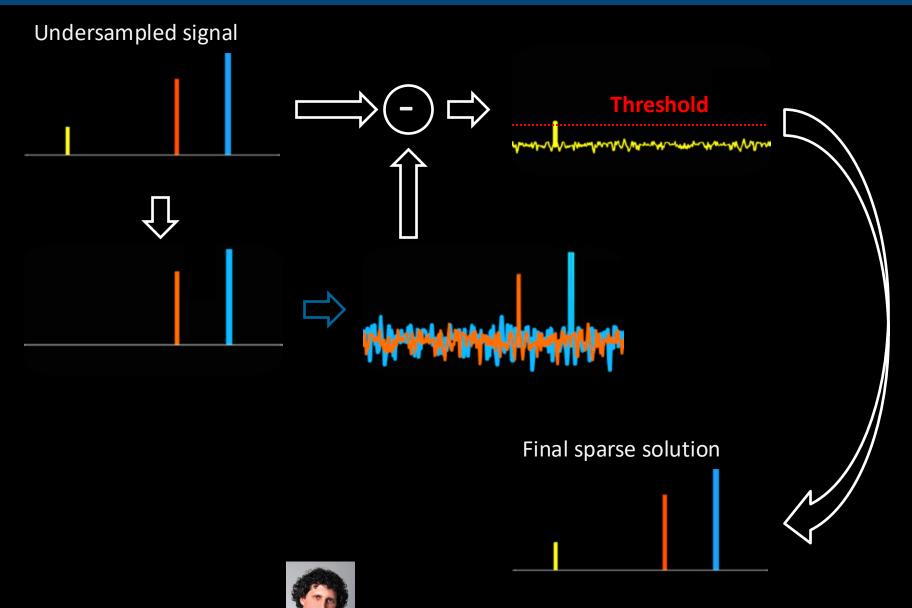
#### Simple compressed sensing example



#### Find sparse solution: Simple iterative algorithm

- Threshold so that 2 largest impulses are preserved
- Apply undersampling
- Subtract from previous signal
- Threshold again

## Simple compressed sensing example



# Sparsity

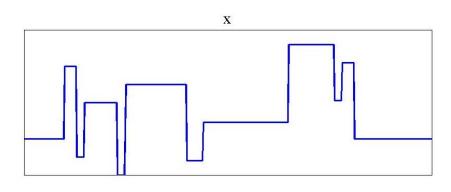
#### Sparsifying transforms

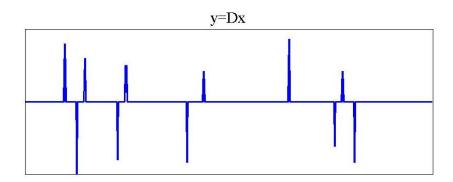
#### Finite differences

$$y(n) = x(n) - x(n-1)$$

In matrix form: y = Dx

$$D = \begin{bmatrix} 1 & -1 & & \\ & 1 & -1 & \\ & & 1 & -1 \end{bmatrix}$$





Total variation

$$TV(x) = \sum_{n=2}^{N} |x(n) - x(n-1)|$$

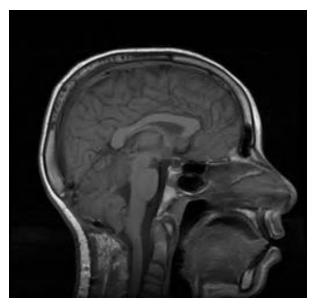


$$\min TV(x) = \min \|Dx\|_{1}$$

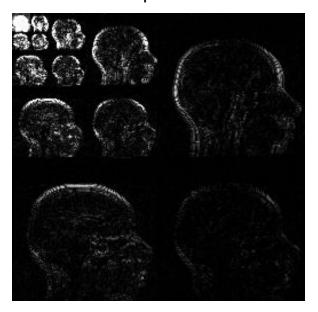
## Sparsifying transforms

- Wavelets
  - Multi-resolution image representation
  - Recursive application of the wavelet function modified by the scaling function (each resolution is twice of that of the previous scale)

Brain image



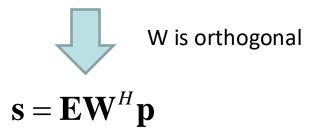
Daubechies 4-tap wavelet transform



## Incoherence

#### Transform Point Spread Function (TPSF)

- Encoding model: s = Em
- Representation model:  $\mathbf{p} = \mathbf{Wm}$  (**p** is sparse)

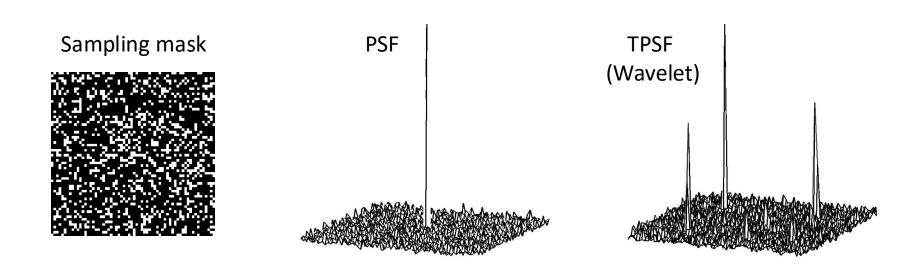


Transform point spread function for position r

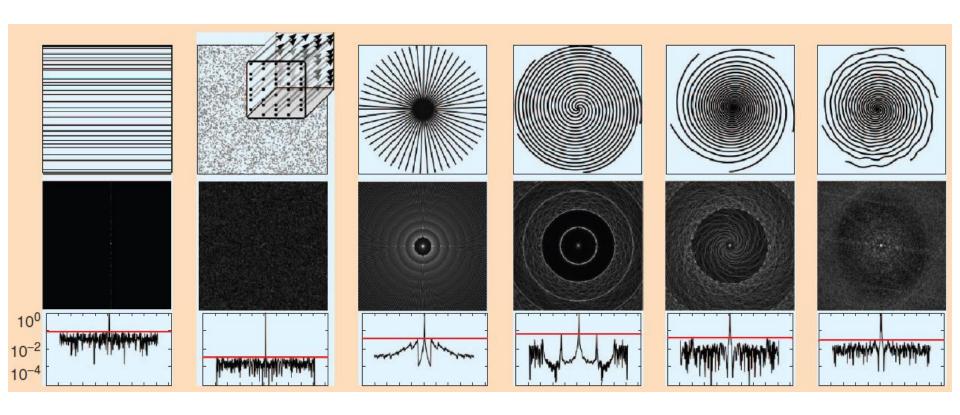
$$TPSF(r) = \mathbf{WE}^H \mathbf{EW}^H_{(r)}$$

#### Transform Point Spread Function (TPSF)

- Tool to check incoherence in the sparse domain
- Computation
  - Apply inverse FFT to sampling mask (1=sampled, 0=otherwise)
  - Apply sparsifying transform
- Incoherence = ratio of the main peak to the std of the pseudo-noise (incoherent artifacts)



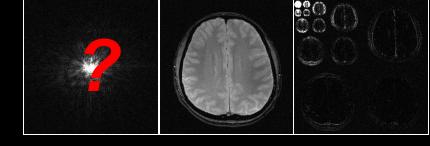
#### Incoherence of k-space trajectories

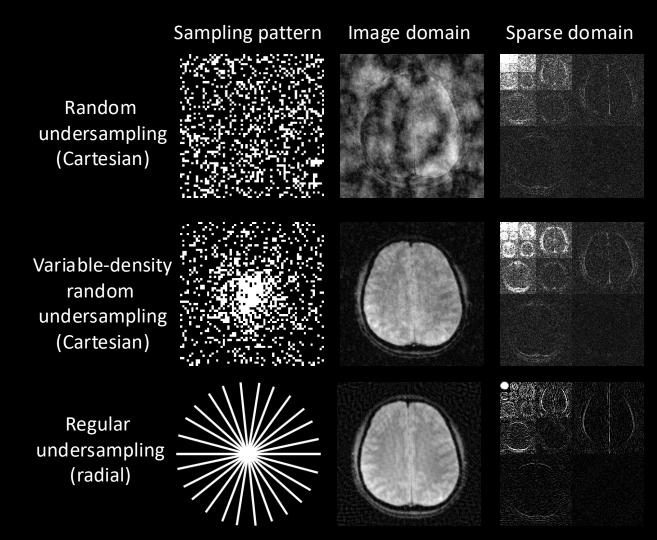


Lustig M, Donoho DL, Santos JM, Pauly JM. Compressed Sensing. MRI, IEEE Signal Processing Magazine, 2008; 25(2): 72-82

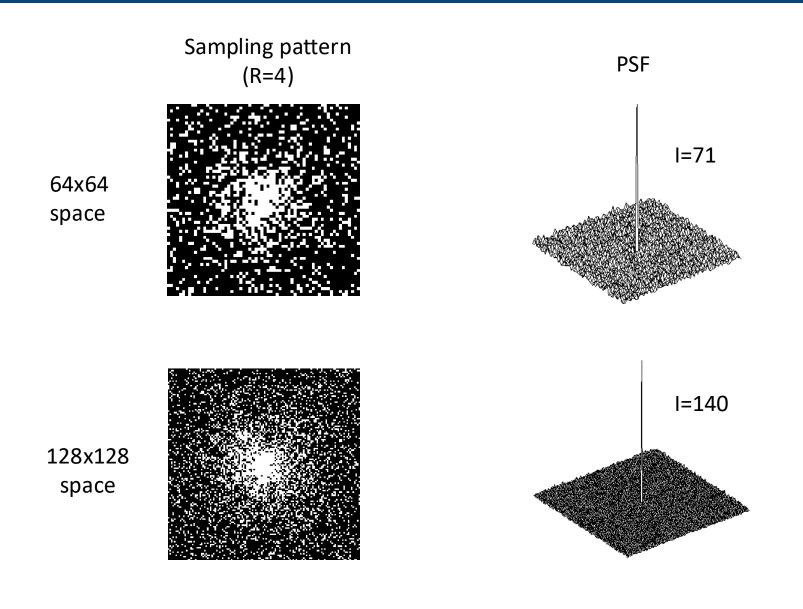
#### Incoherent sampling patterns

• What are the best samples?





## Dimensionality and incoherence



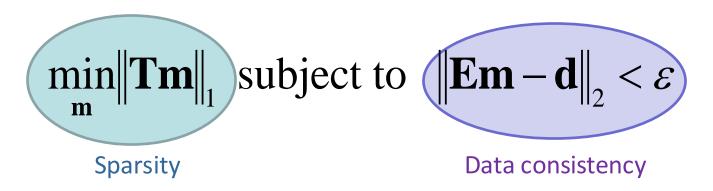
# Sparse reconstruction

#### Compressed sensing reconstruction

 $\hbox{ \bullet Acquisition model: } d = Em \qquad \begin{array}{|l|l|l|} \hbox{ d : acquired data} \\ \hbox{ E : undersampled Fourier transform} \\ \end{array}$ 

m: image to reconstruct

• Sparsifying transform:  ${f T}$ 



$$\|\mathbf{x}\|_1 = \sum_{i=1}^N |x_i|$$
 ( $I_1$ - norm of  $\mathbf{x}$ )

#### Compressed sensing reconstruction

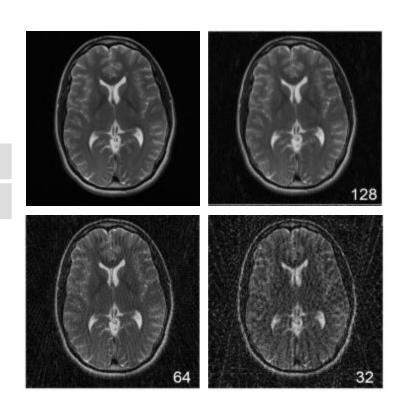
Unconstrained optimization (in practice)

$$\min_{\mathbf{m}} \left\| \mathbf{Em} - \mathbf{d} \right\|_{2}^{2} + \lambda \left\| \mathbf{Tm} \right\|_{1}$$

- Regularization parameter  $\lambda$ 
  - Trade-off between data fidelity and removal of aliasing artifacts
  - High  $\lambda$ : artifact removal and denoising at the expense of image corruption (blurring, ringing, blocking, etc)
  - Low  $\lambda$ : no image corruption, but residual aliasing

#### Example: TV Norm, radial subsampling

Data set	Total Variation (a.u.)
Original (256×256)	2801



Rudin et al., Phys. D 60: 259-268 (1992) Block et al., MRM 57: 1086-1098 (2007) Knoll et al., MRM 65: 480-491 (2011) Knoll et al., MRM 67: 43-41 (2012)

#### Compressed sensing reconstruction

Gradient descent

- Cost function: 
$$C(\mathbf{m}) = \|\mathbf{Em} - \mathbf{d}\|_{2}^{2} + \lambda \|\mathbf{Tm}\|_{1}$$

- Iterations:  $\mathbf{m}_{n+1} = \mathbf{m}_n - \alpha \nabla C(\mathbf{m}_n)$ 

$$\nabla C(\mathbf{m}_n) = 2\mathbf{E}^H (\mathbf{E}\mathbf{m}_n - \mathbf{d}) + \lambda \mathbf{T}^H \mathbf{M}^{-1} \mathbf{T}\mathbf{m}_n$$

M is a diagonal matrix: 
$$M_{ii} = \sqrt{(\mathbf{Tm})_i^*(\mathbf{Tm})_i^* + \mu}$$

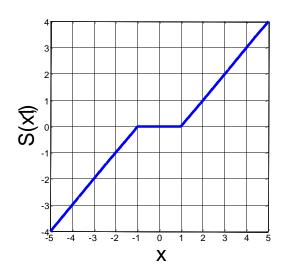
Approximate assumption: Regularized I1 norm

$$|x| = \sqrt{x^* x + \mu}$$

#### Compressed sensing reconstruction

- Proximal gradient descent (iterative soft-thresholding)
  - Soft-thresholding operation

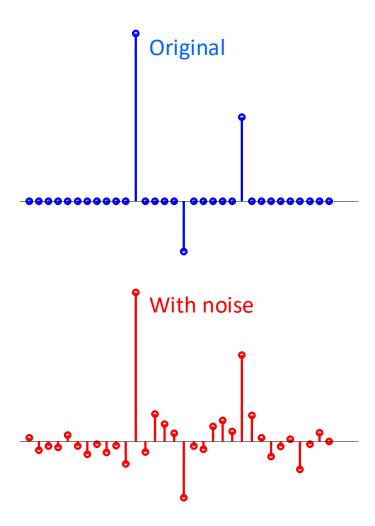
$$S(x,\lambda) = \begin{cases} 0, & \text{if } |x| \le \lambda \\ \frac{x}{|x|} (|x| - \lambda), & \text{if } |x| > \lambda \end{cases}$$



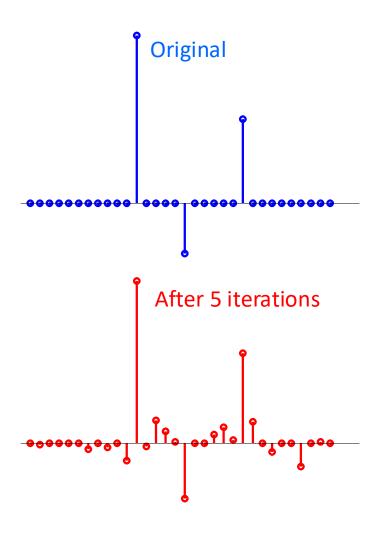
Our gradient gradient-descent algorithm becomes

$$\mathbf{m}_{n+1} = \mathbf{T}^{-1} \left[ S \left( \mathbf{T} \left[ \mathbf{m}_{n} - \mathbf{E}^{H} \left( \mathbf{E} \mathbf{m}_{n} - \mathbf{d} \right) \right], \lambda \right) \right]$$

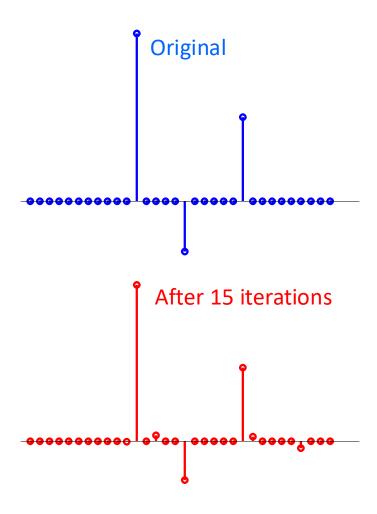
Sparse signal denoising



Sparse signal denoising

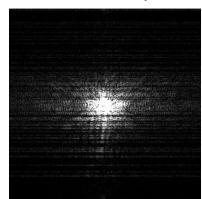


Sparse signal denoising



#### **Initial solution**

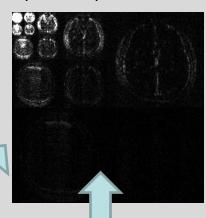
Inverse FT of the zero-filled k-space

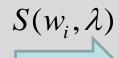




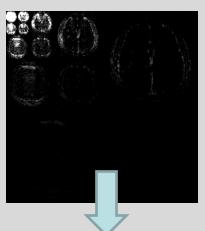
#### **Iterations**

Sparse representation

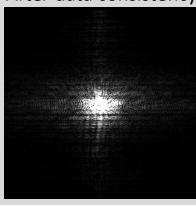




After soft-thresholding

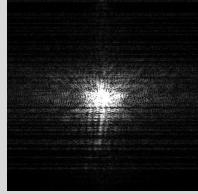


After data consistency





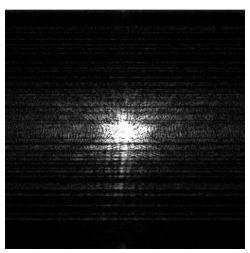
k-space representation



#### Iterative soft-thresholding (R=3)

**Initial solution** 

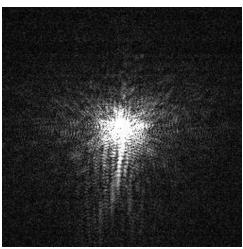
Inverse FT of the zero-filled k-space

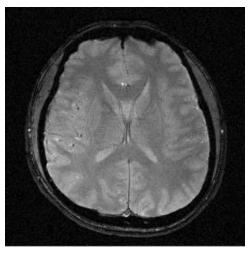




**After 30 iterations** 

Iterative soft-thresholding

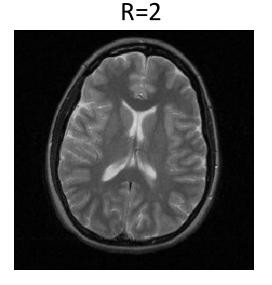


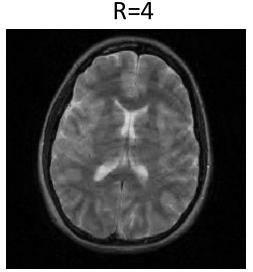


#### Image quality in compressed sensing

SNR is not a good metric

- Loss of small coefficients in the sparse domain
  - Loss of contrast
  - Blurring
  - Blockiness
  - Ringing
  - Images look more synthetic





# Combination of compressed sensing and parallel imaging

#### Why would CS & PI make sense?

 Image sparsity and coil-sensitivity encoding are complementary sources of information

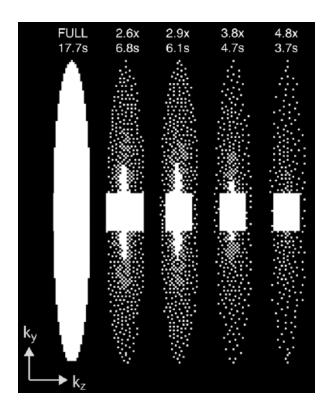
Compressed sensing can regularize the inverse problem in parallel imaging

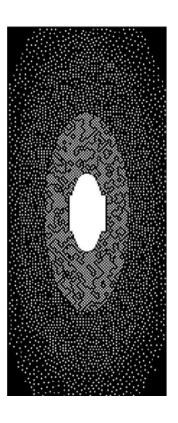
Parallel imaging can reduce the incoherent aliasing artifacts

## Challenges of CS & PI?

 CS requires irregular k-space sampling while PI requires regular k-space sampling

#### Poisson disk sampling





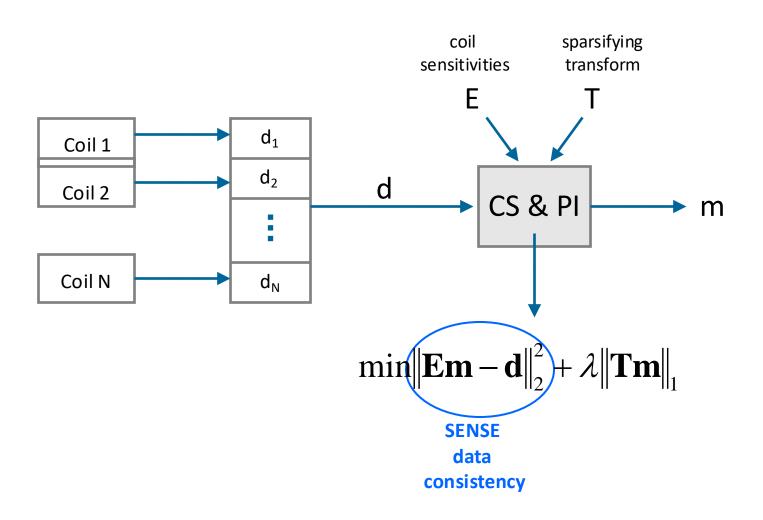
#### Approaches for CS&PI

- CS with SENSE parallel imaging model
  - Multicoil imaging with variational regularization
- CS with GRAPPA parallel imaging model
  - $-I_1$ -SPIRiT

Block et al. MRM 2007 Knoll et al. MRM 2011 Lustig M et al. MRM 2010

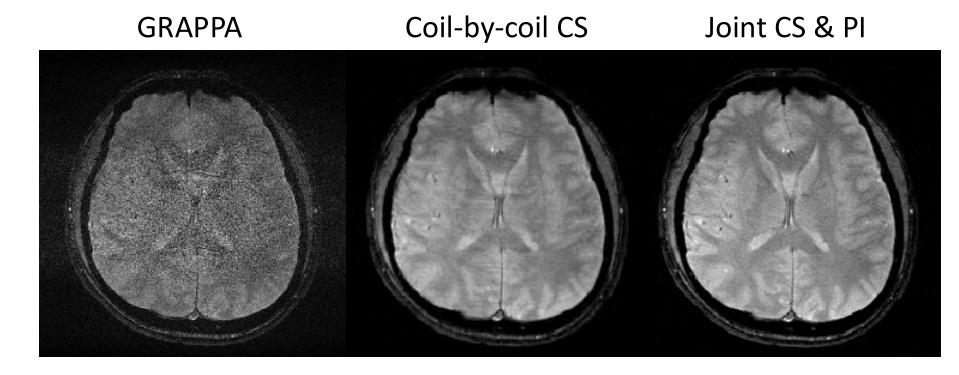
#### CS with SENSE parallel imaging model

Include parallel imaging in data consistency term



#### CS & PI for 2D imaging

- Siemens 3T Tim Trio
- 12-channel matrix coil array
- 4-fold acceleration



#### Summary

- Compressed sensing
  - New sampling theorem
    - Information rate rather than pixel rate
  - Ingredients
    - Sparsity
    - Incoherence
    - Non-linear reconstruction

- Fast imaging tool for MRI
  - MR images are naturally compressible
  - Data acquisition in k-space facilitates incoherence
  - Can be combined with parallel imaging