

# Spiking and firing rate resonance in single neurons: dynamic mechanisms of communication of subthreshold resonance to the spiking regime

Introduction to modeling and data analysis tools to capture resonance phenomena (2nd class)

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Rodrigo F. O. Pena

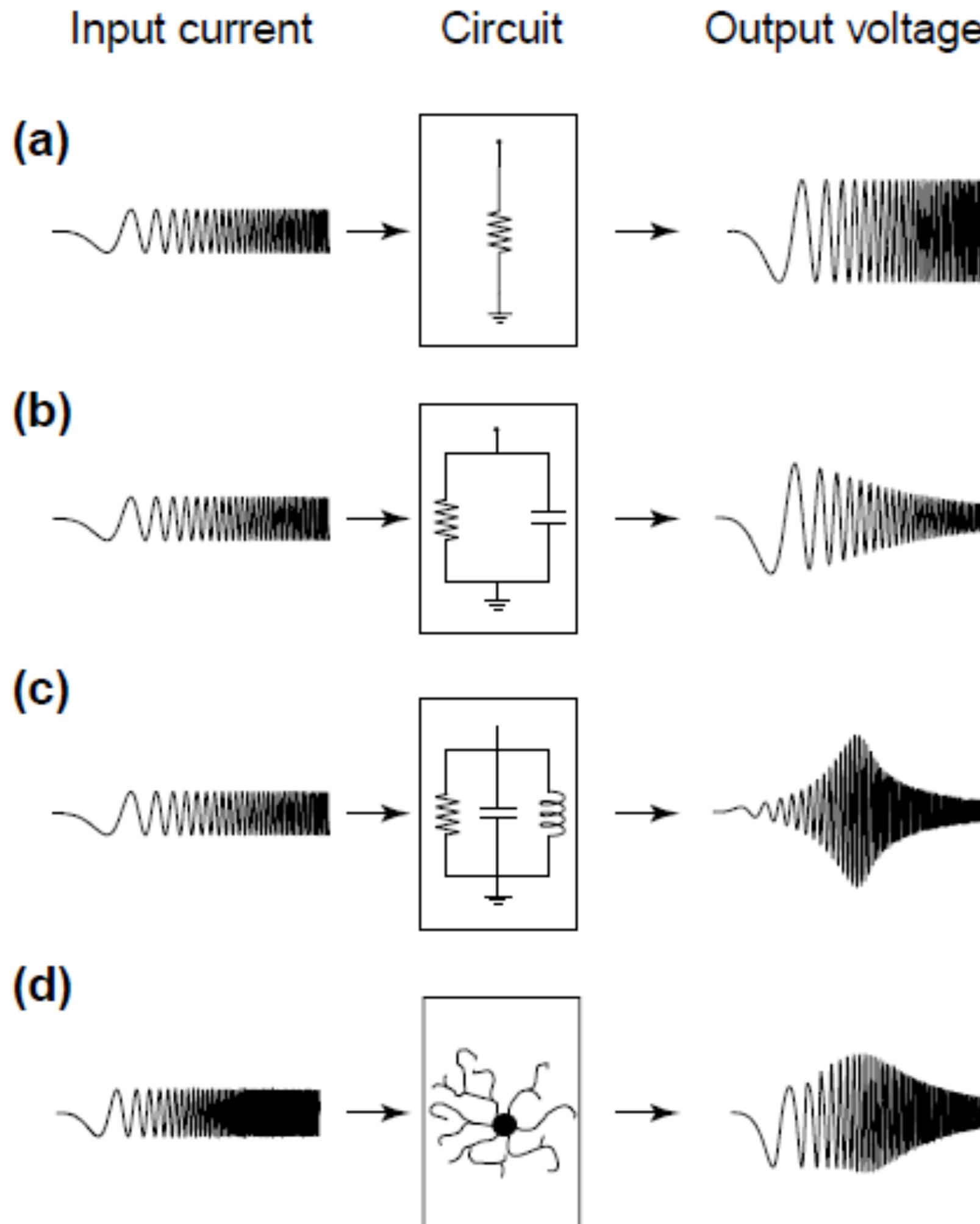
New Jersey Institute of Technology and Rutgers University

15/10/2020



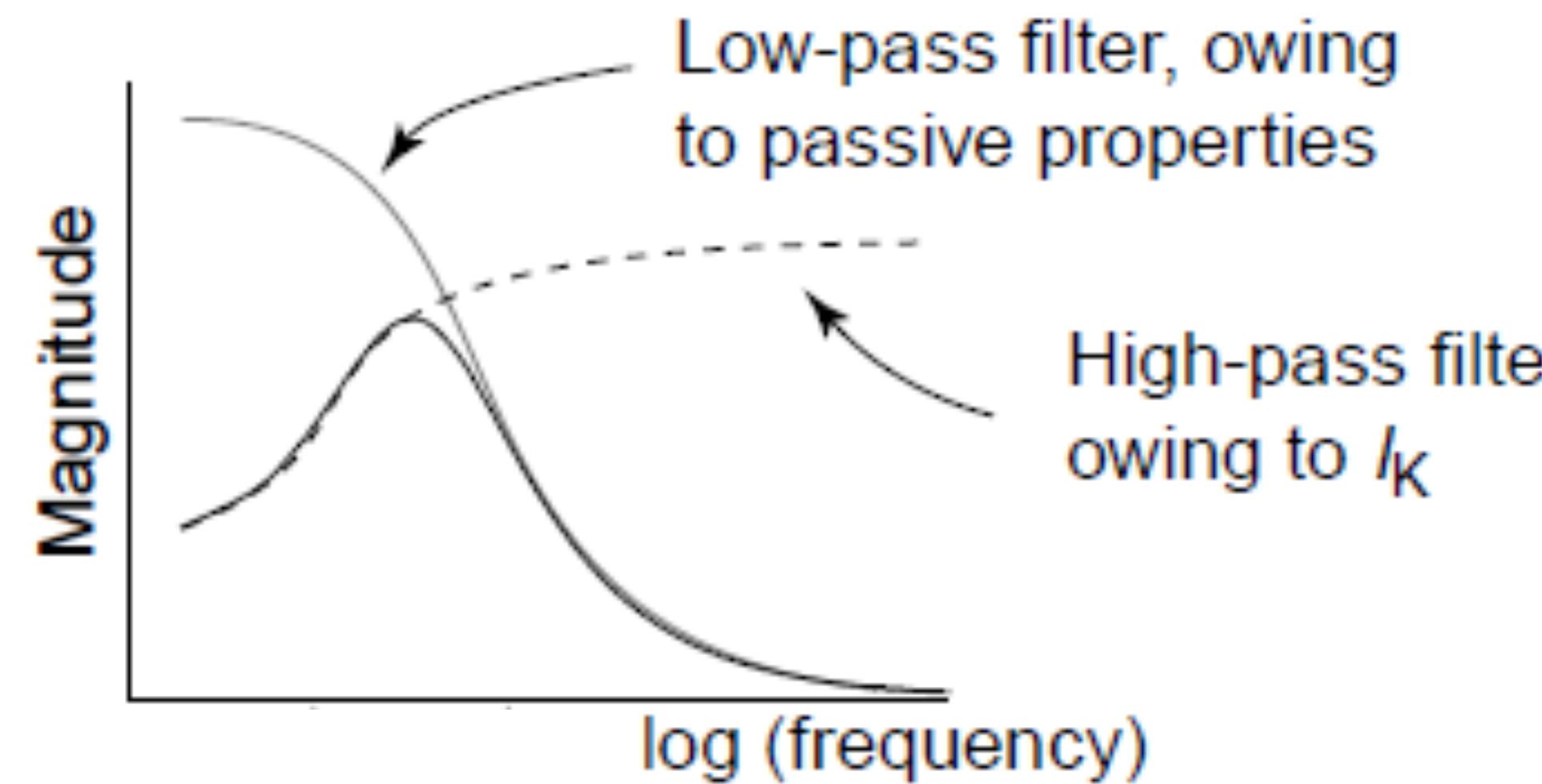
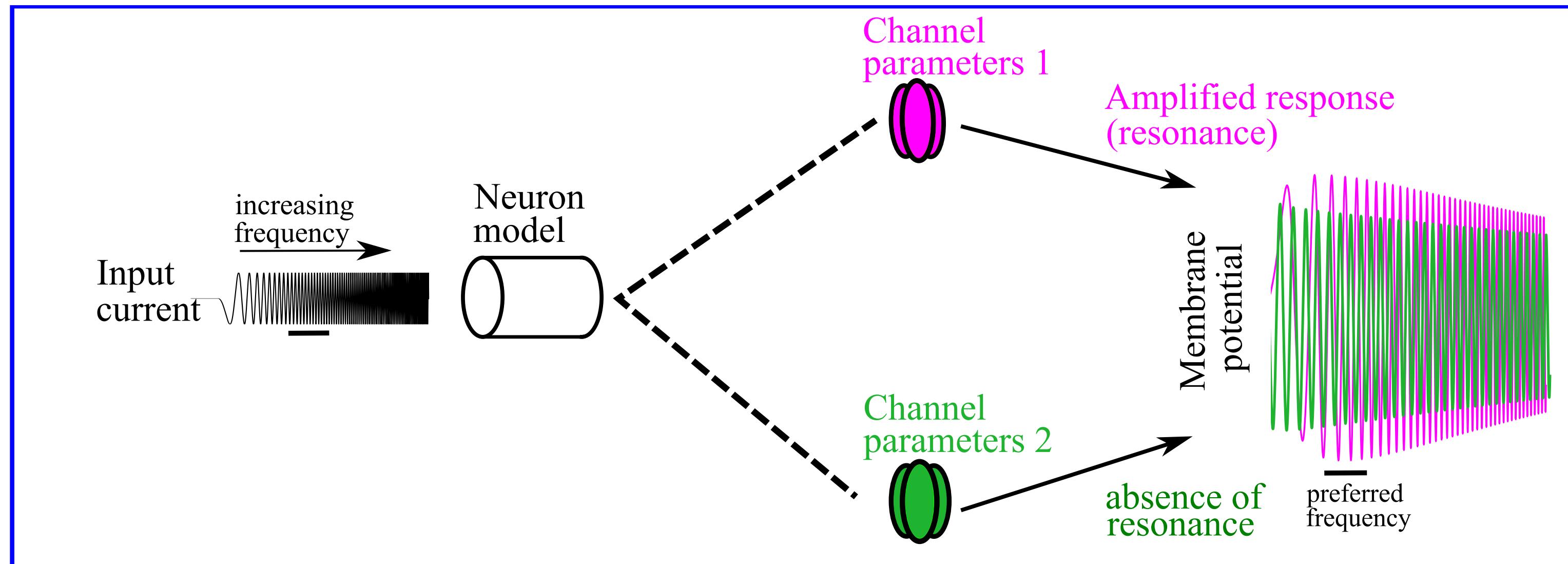
# Resonance in electrical circuits

Chirp input



Hutcheon & Yarom (2000)  
*Trends Neurosci.* 23:216-22

# What determines sub threshold resonance in neurons?



Hutcheon & Yarom,  
*Trends Neurosci* (2000) 23:216-22

# What determines sub threshold resonance in neurons?

- interplay of positive and negative feedback effects

**slow restorative ionic currents (resonant)**

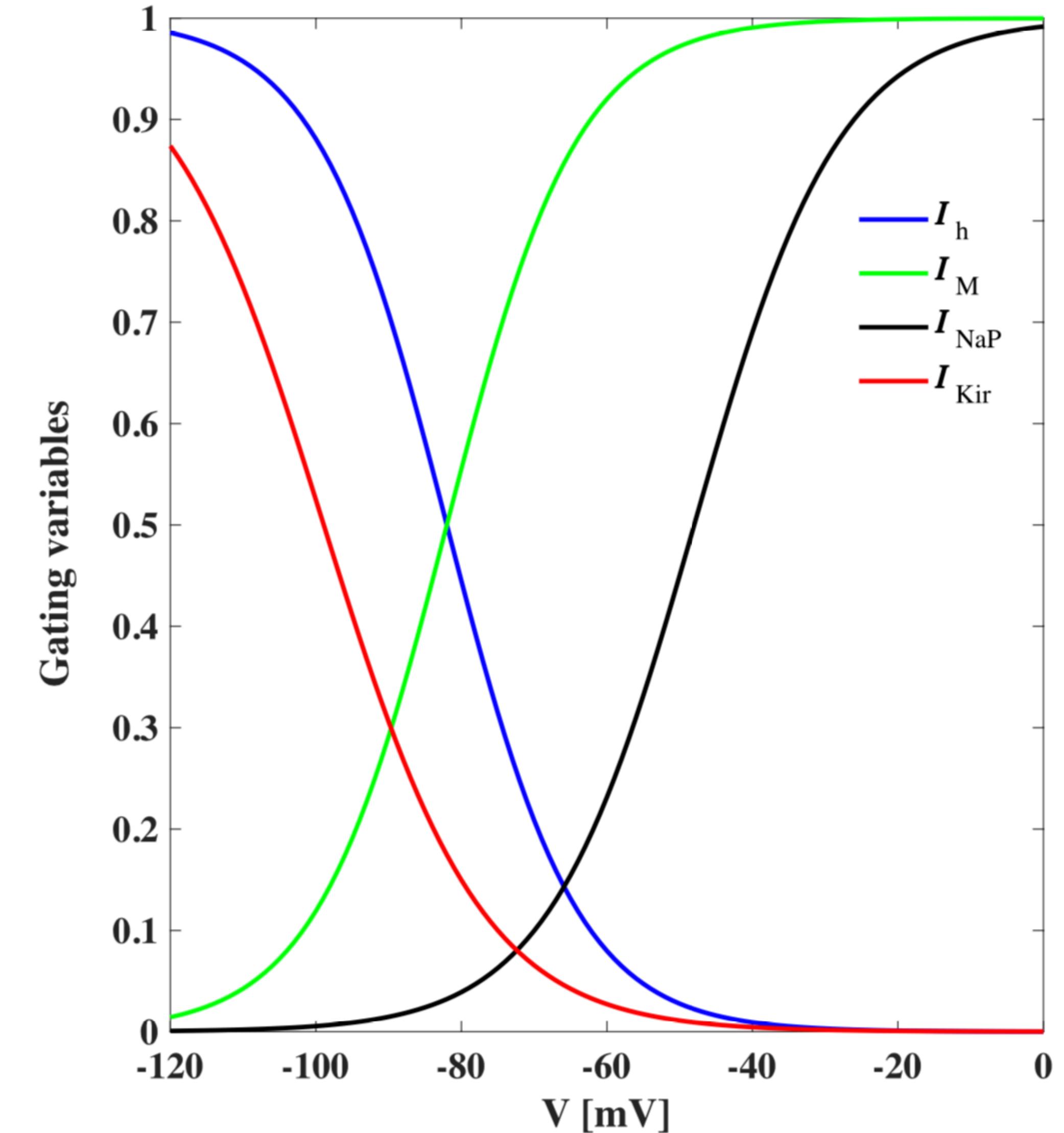
$I_h$  (hyperpolarization-activated mixed-cation)

$I_M$  (M-type slow-potassium)

**regenerative currents (amplifying)**

$I_{NaP}$  (persistent sodium)

$I_{Kir}$  (inward-rectifying potassium)



Pena et al., *Chaos* **29**, 103135 (2019)

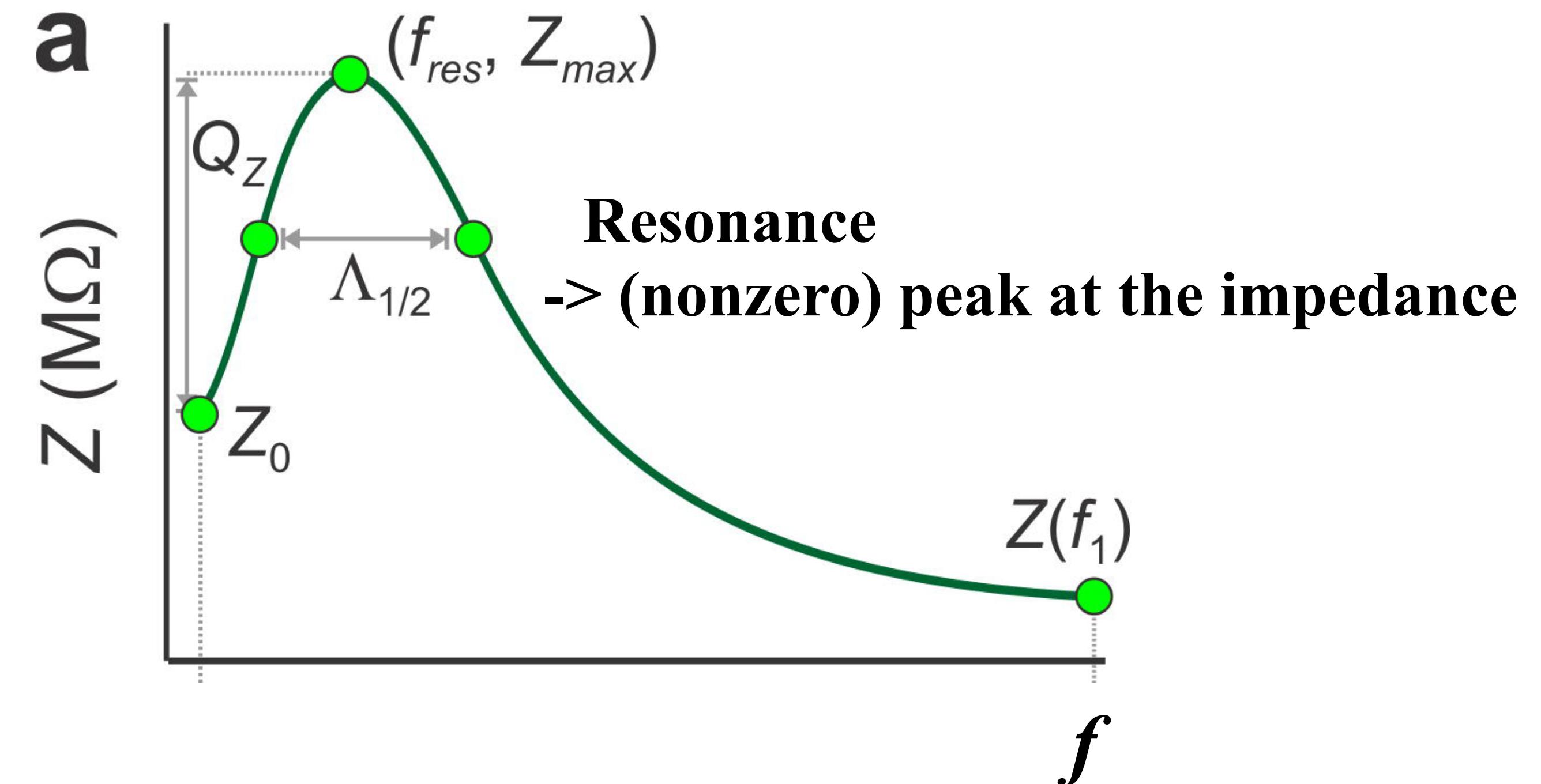
# The impedance profile

The impedance

$$Z(f) = \frac{FFT[V_{out}(t)]}{FFT[I_{in}(t)]}$$

For a **nonlinear system**, or **linear systems with non-sinusoidal inputs**,

$$Z(f) = \frac{V_{max}(f) - V_{min}(f)}{2A_{in}}$$



Fox et al., *PLoS Comput Biol* (2017) 13: e1005565.

Assumption: output is periodic and has the same frequency as the input!

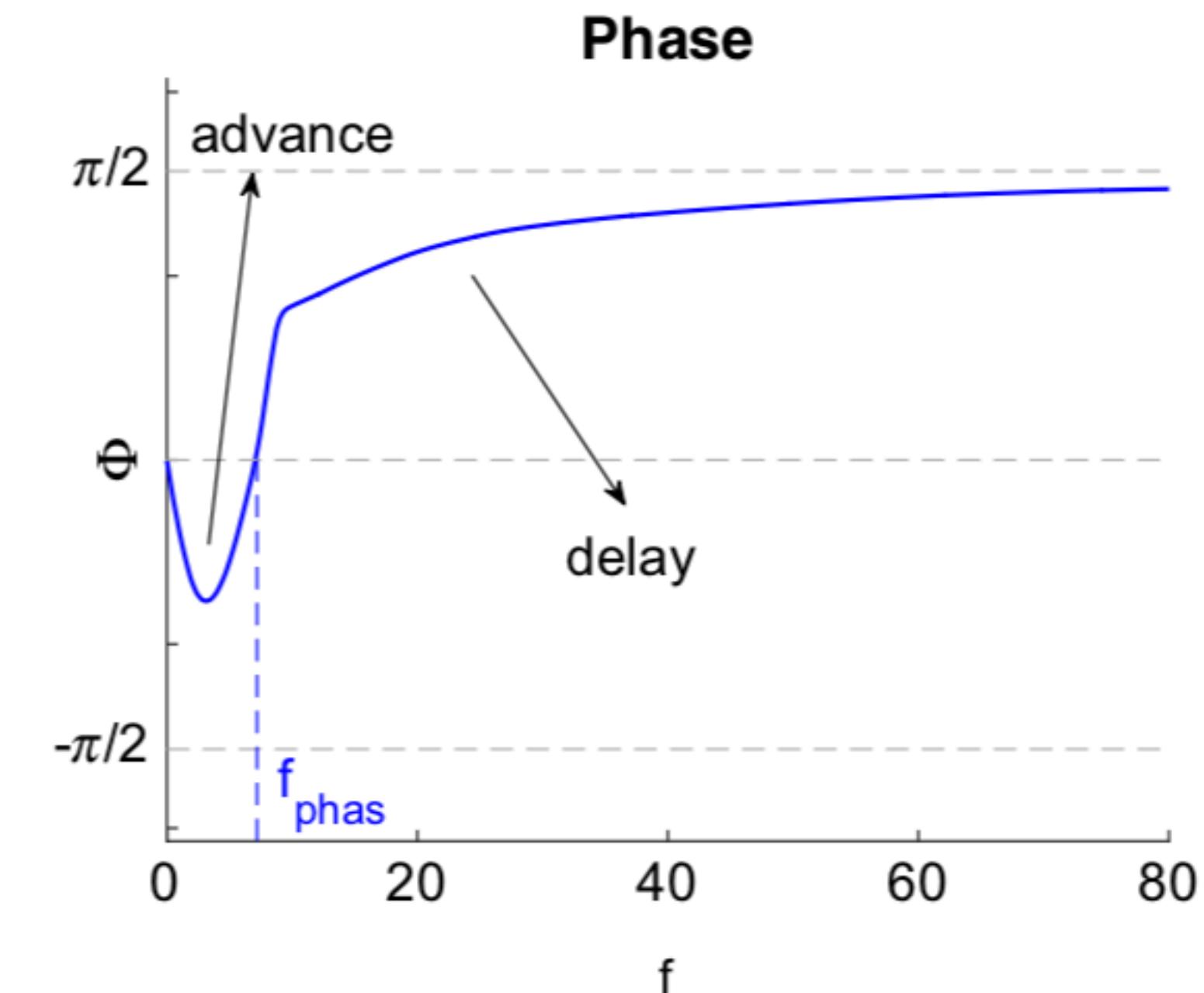
# The phase-shift profile

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The phase  $\phi(f)$

$$\phi(f) = -\tan^{-1} \left( \frac{Z_{imag}(f)}{Z_{real}(f)} \right)$$

$$\phi(f) = \frac{t_{peak,out}(f) - t_{peak,in}(f)}{T_{per}(f)}$$

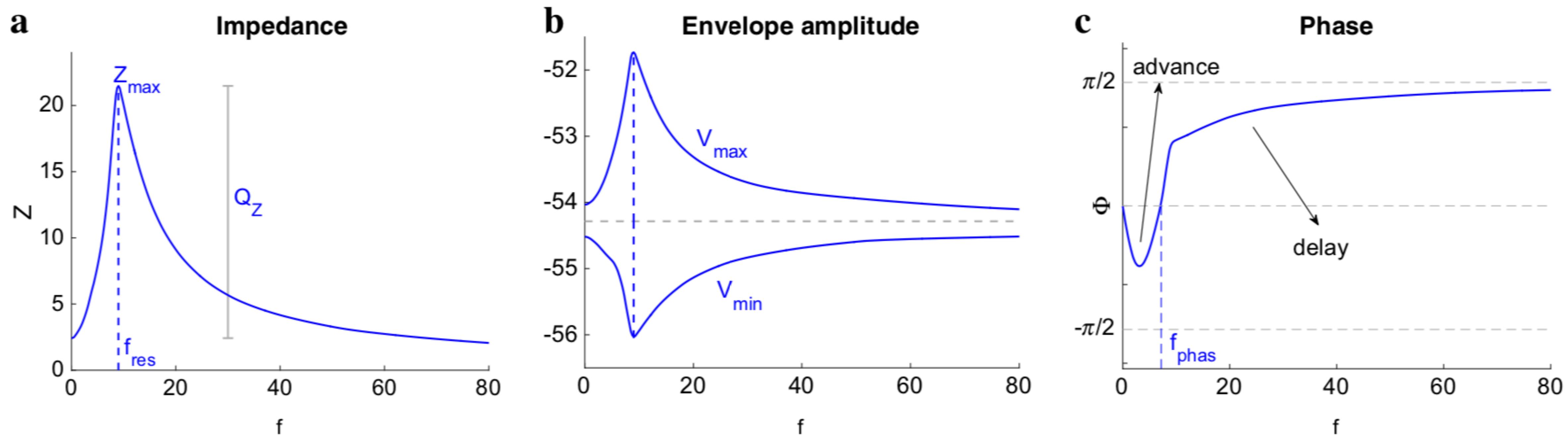


**Phasonance:**

-> phase profile vanishes at a nonzero input frequency!

Rotstein, *J Comput Neurosci* (2017) 43:243–271

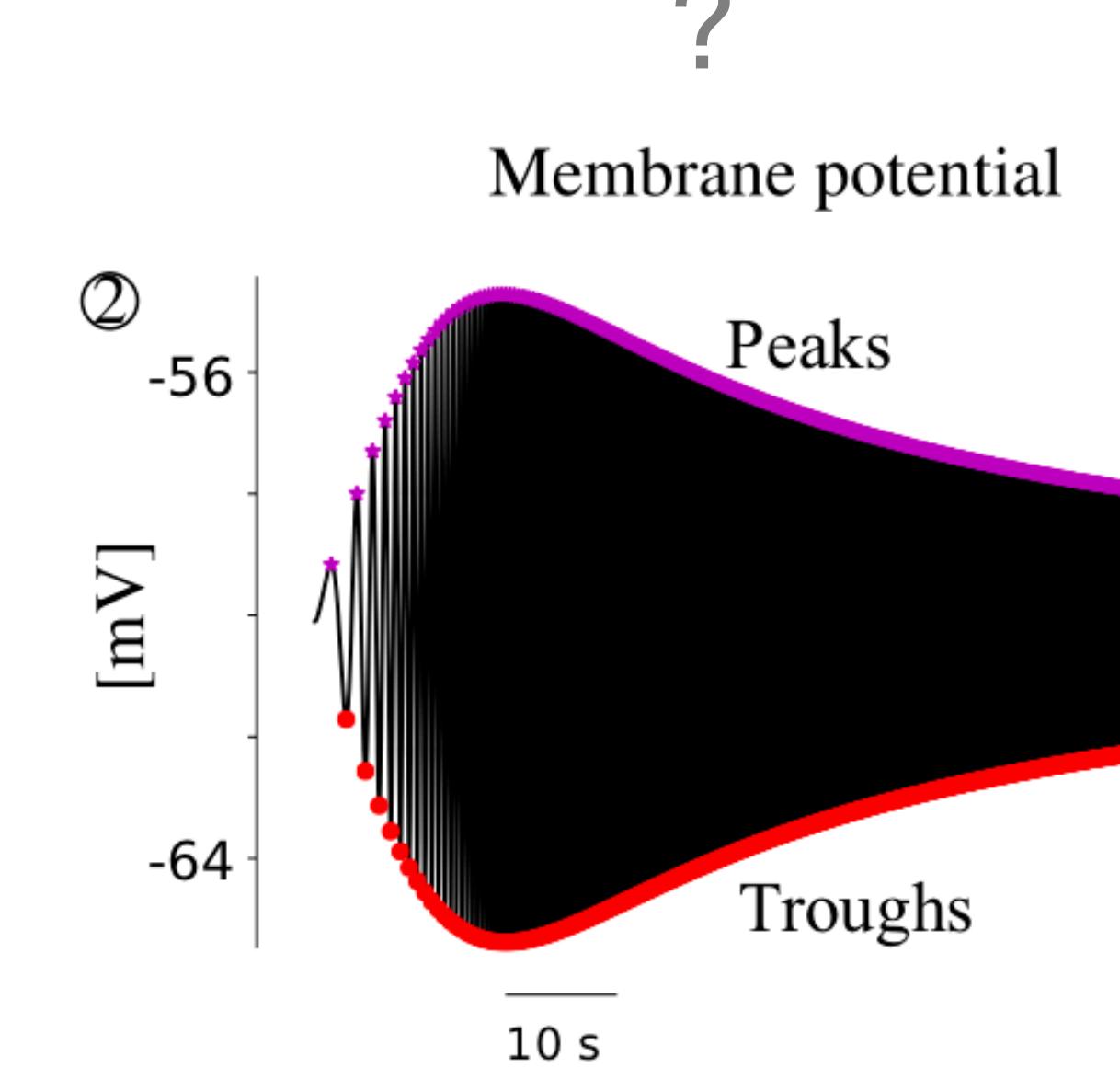
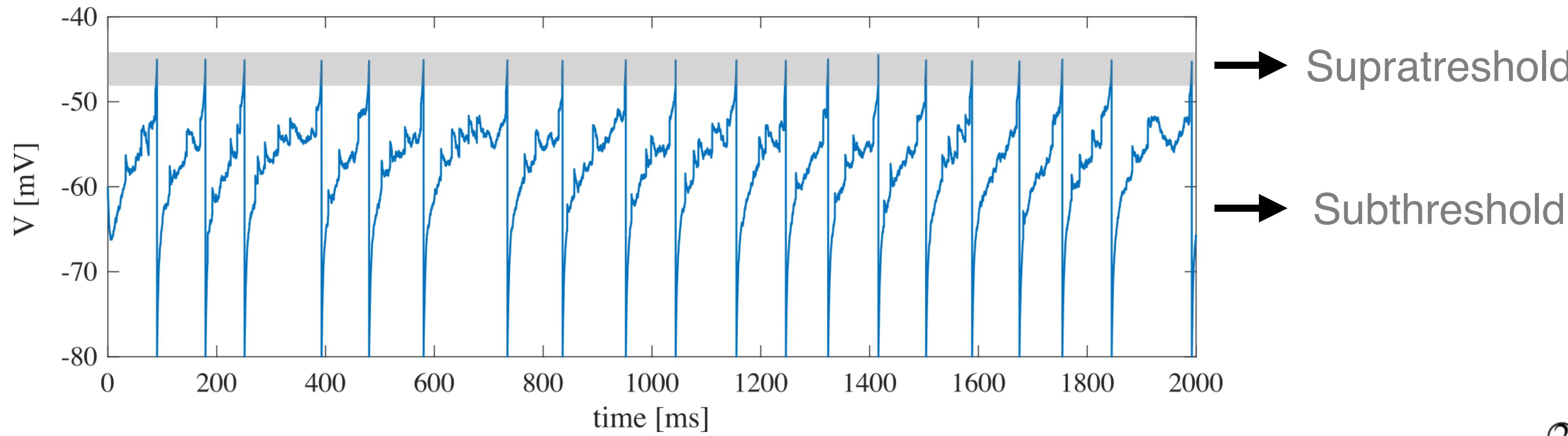
# Basic resonance characteristics — subthreshold behavior

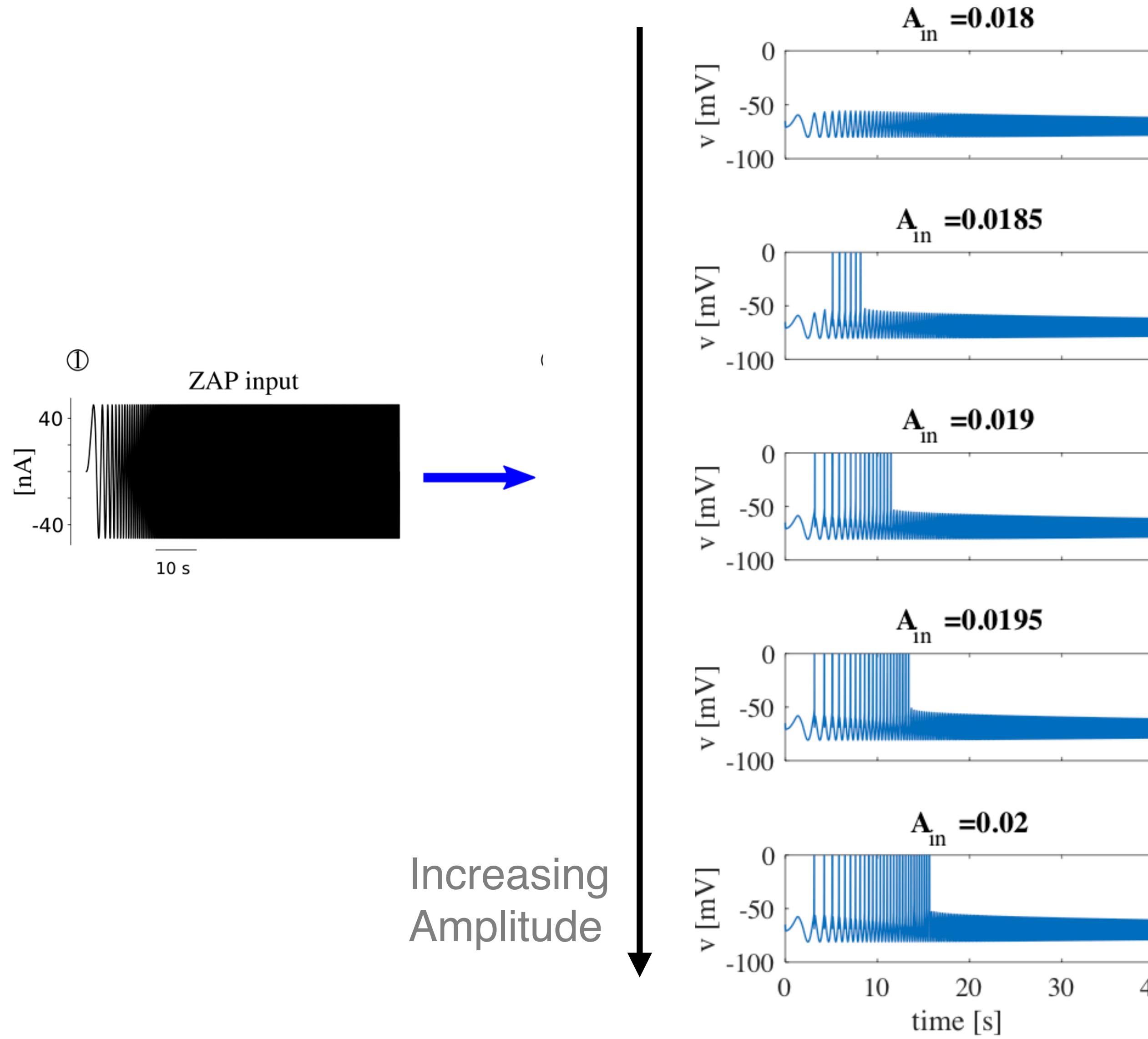


Rotstein, *J Comput Neurosci* (2017) 43:243–271

# How to connect subthreshold to spiking behavior

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Impedance profile when spikes are present?

Is subthreshold resonance communicated to the suprathreshold regime?

Important questions for theta (4-11 Hz) oscillations!

Mechanism that may contribute to theta generation: the resonant properties of neurons.

# Outline

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- Resonance for **suprathreshold** (spiking) behavior vs. **subthreshold regime (upper envelope)**;
- Resonance for **suprathreshold** (spiking) behavior vs. subthreshold regime (**bottom envelope**);
- **Subthreshold** resonance when a neuron is **driven by spikes**.

# Outline

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- Resonance for **suprathreshold** (spiking) behavior vs. **subthreshold regime (upper envelope)**;
  - Single neuron and relation to dynamics [Rotstein, *J Comput Neurosci* (2017) 43:243–271]
  - Population [Richardson et al., *J Neurophysiol* (2003) 89:2538–2554]
- Resonance for **suprathreshold** (spiking) behavior vs. subthreshold regime (**bottom envelope**);
- **Subthreshold** resonance when a neuron is **driven by spikes**.

# Dynamics (briefly!)

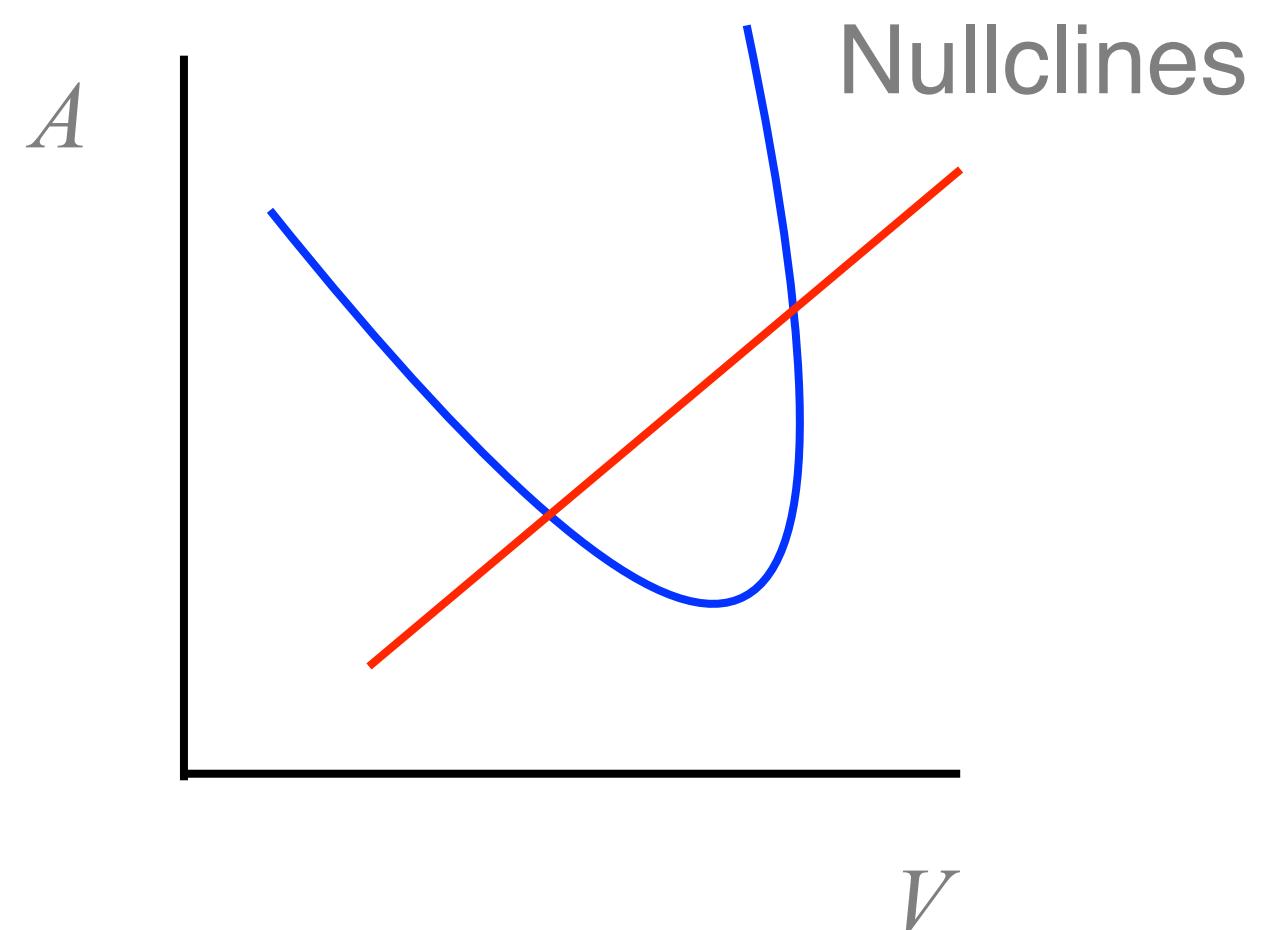
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$$C_m \frac{dV(t)}{dt} = - \sum_i I_i(V, t) - I_{\text{leak}}(V) + I_{\text{ZAP}}(t) + I_{\text{DC}} = 0$$

$$I_i = \bar{g}_i A_i(V, t) (V - E_i)$$

$$\frac{dA_i(V, t)}{dt} = \frac{A_i^\infty(V) - A_i(V, t)}{\tau_i} = 0$$

$$A_i^\infty(V) = \frac{1}{1 + \exp\left(\frac{s(V - V_{1/2})}{k}\right)}$$



# Two very similar models

## **$I_{\text{NaP}}+I_h$ model**

$$C \frac{dV}{dt} = -I_L - I_h - I_{\text{Nap}} + I_{\text{app}} + I_{\text{in}}(t)$$

$$I_L = G_L (V - E_L)$$

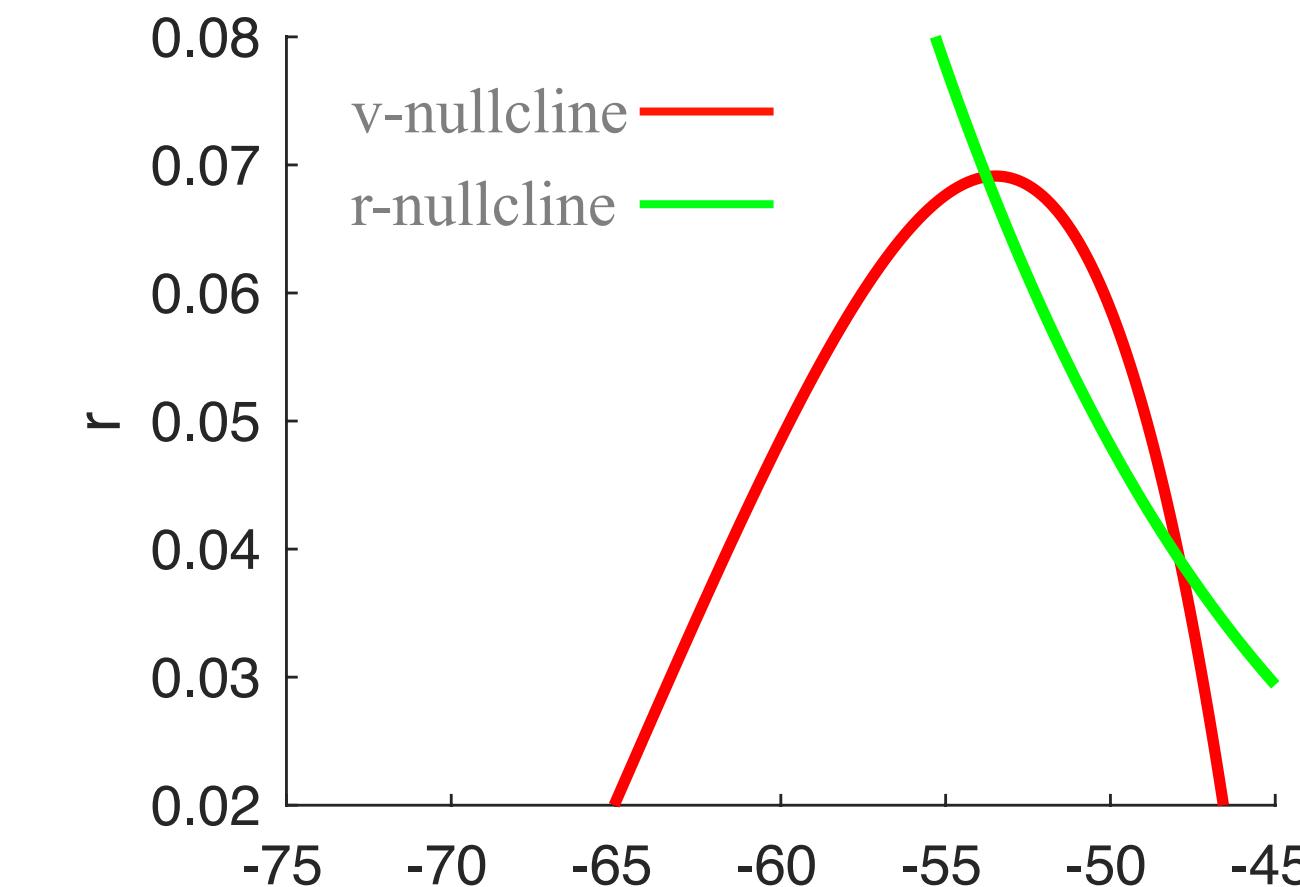
$$I_h = G_h r (V - E_h)$$

$$I_{\text{NaP}} = G_p p_\infty(V) (V - E_{\text{Na}})$$

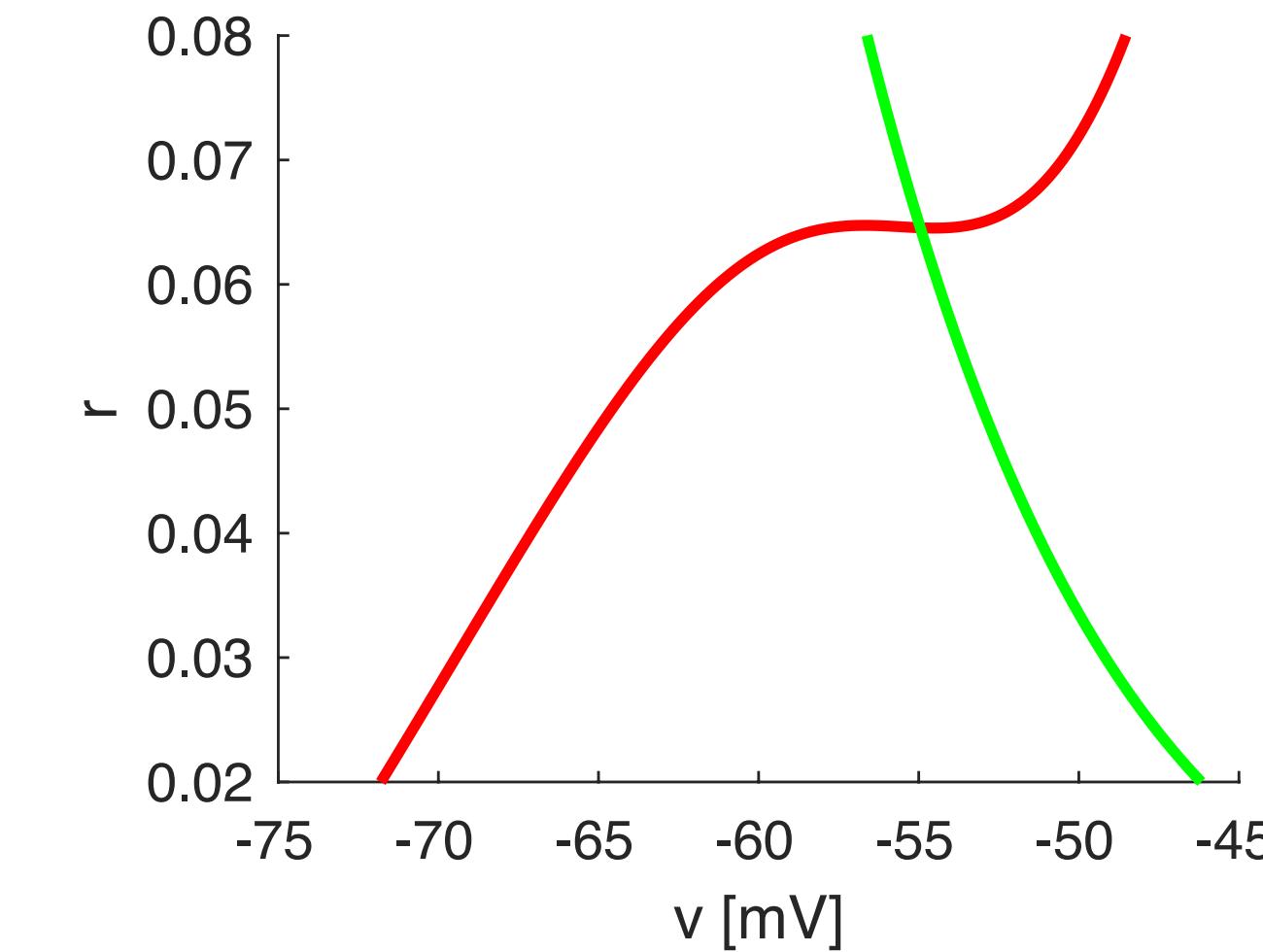
$x$  ( $= r, p$ )

$$\frac{dx}{dt} = \frac{x_\infty(V) - x}{\tau_x(V)}$$

Model 1



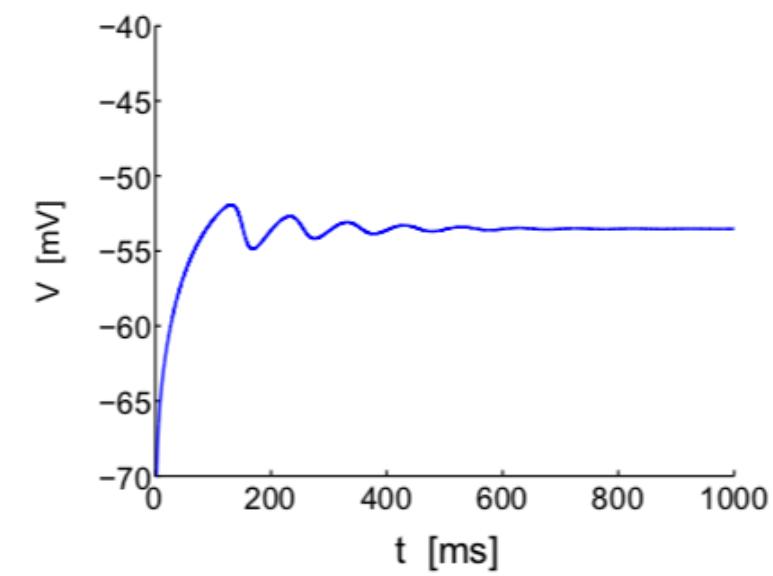
Model 2



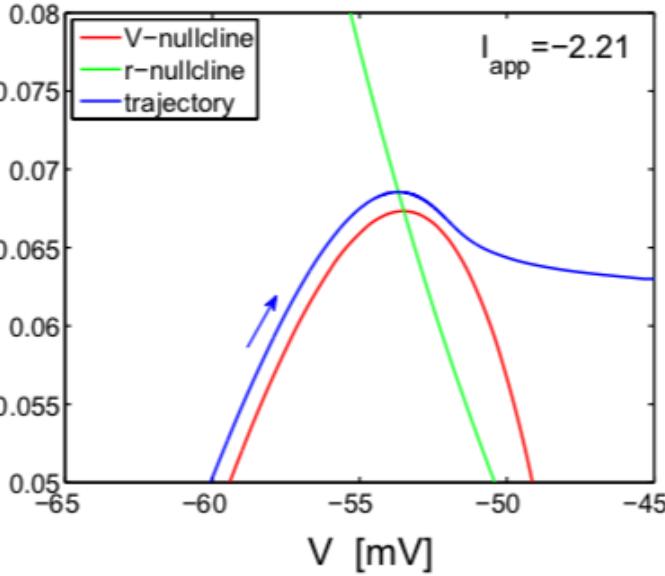
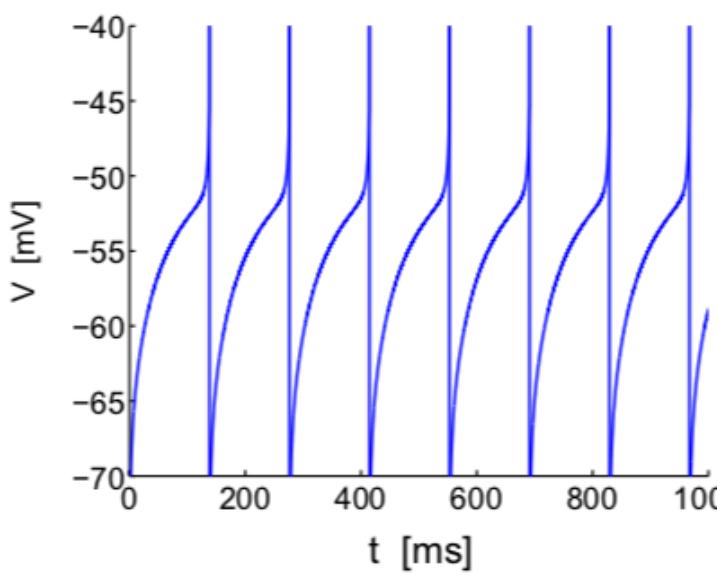
# From subthreshold to spikes

**Model 1**

**a1**



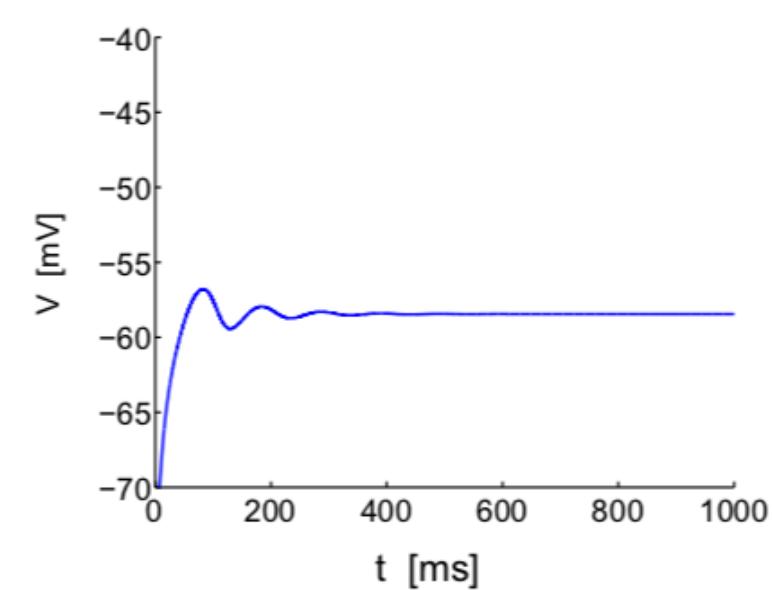
**a2**



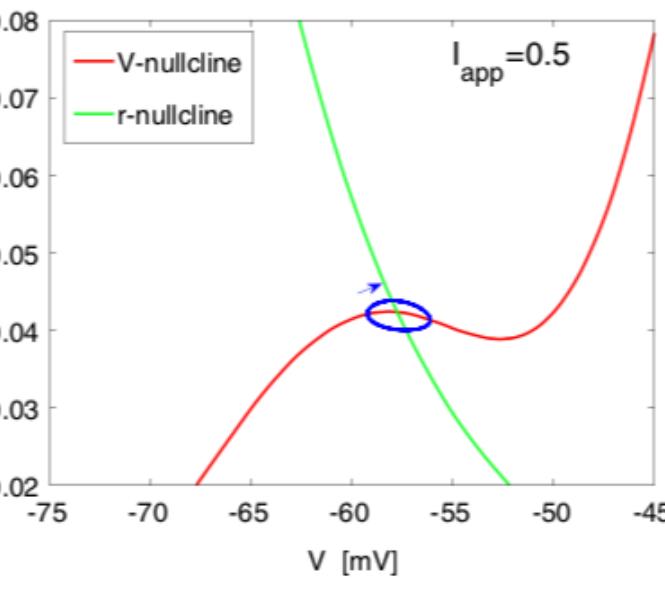
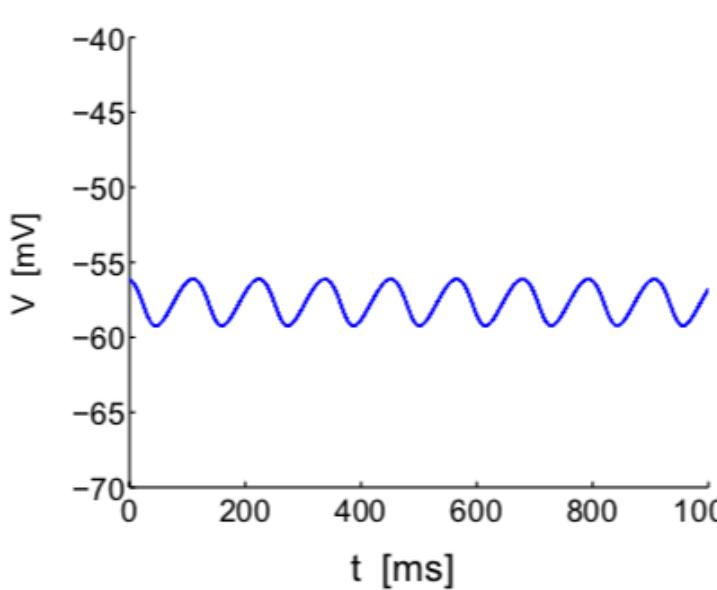
Differences:

- Geometry: parabolic- and cubic-like
- Generation of STOs in the parabolic- and cubic-like
- Transition from STOs to spikes

**b1**

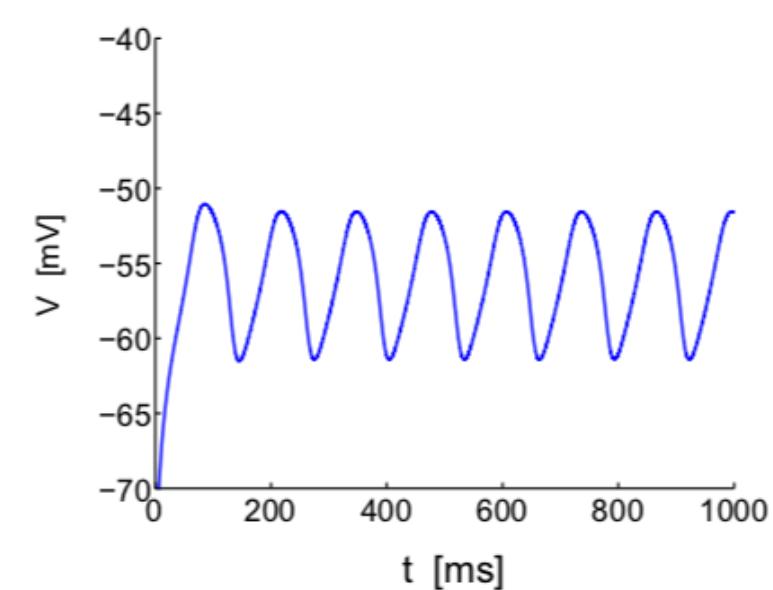


**b2**

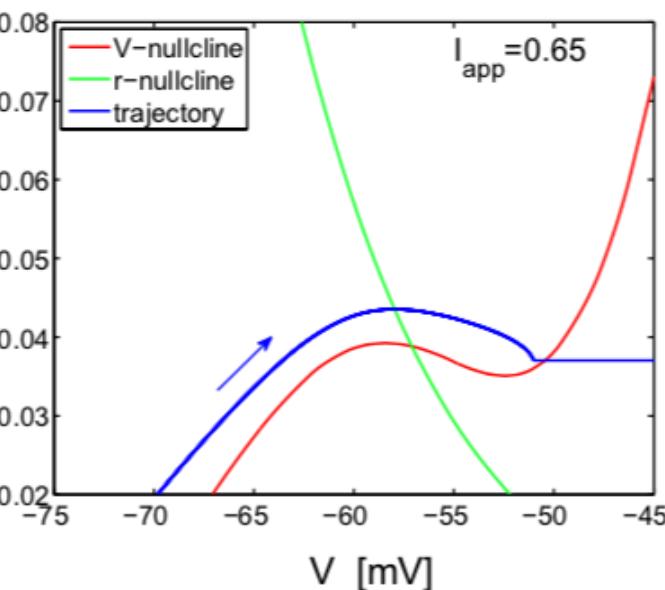
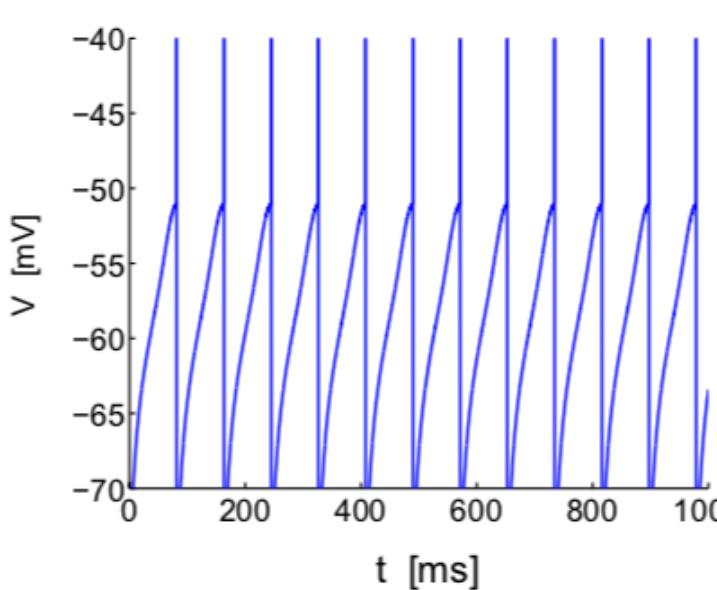


→ **model 1** generates damped STOs but not persistent (unless noise is present).

**b3**



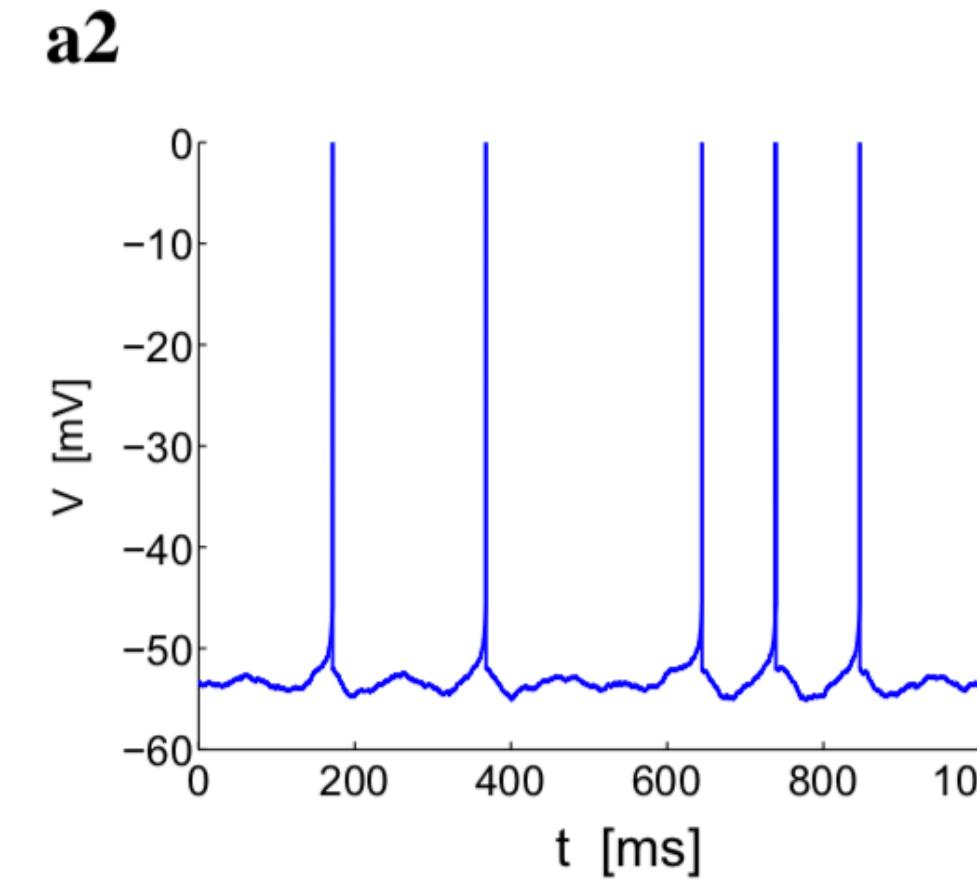
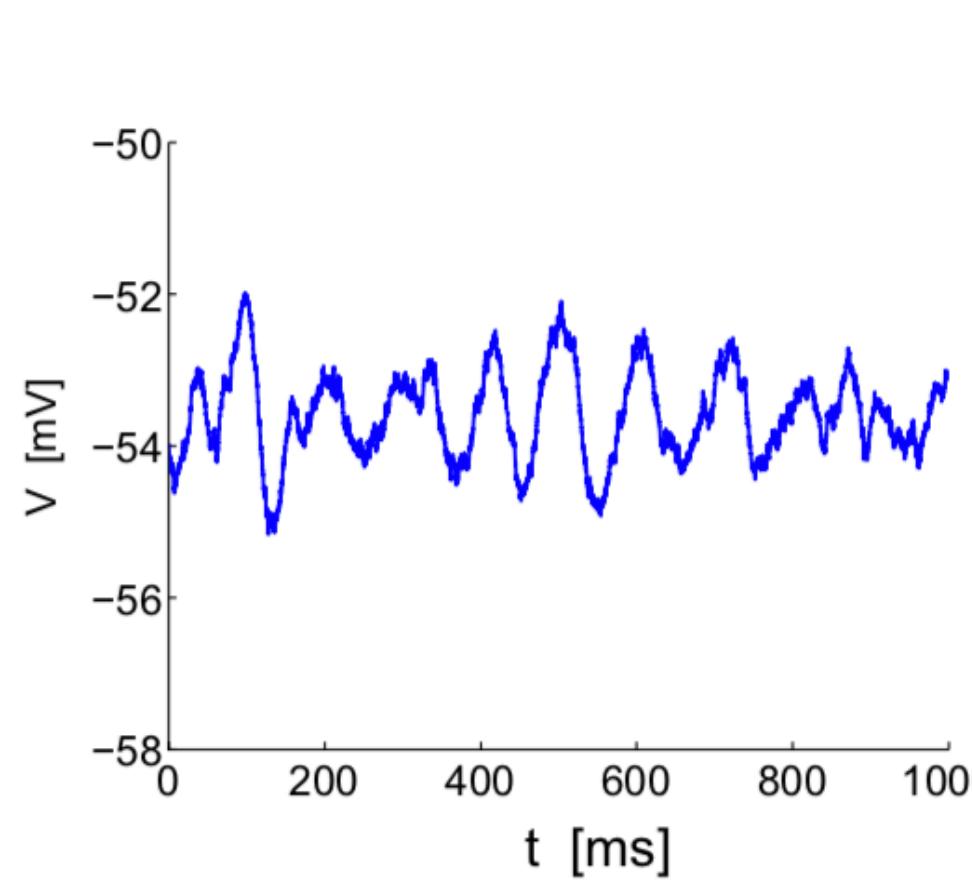
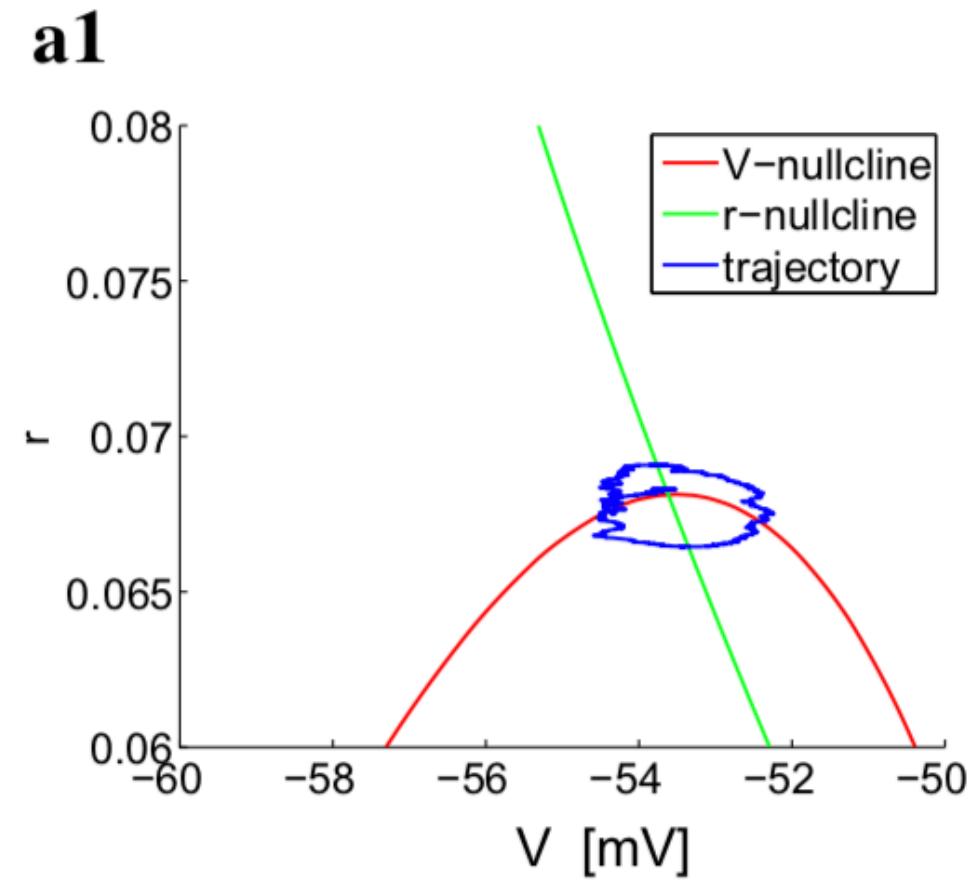
**b4**



→ **model 2** generates persistent STOs  
No mechanism for the onset of spikes.

# From subthreshold to spikes

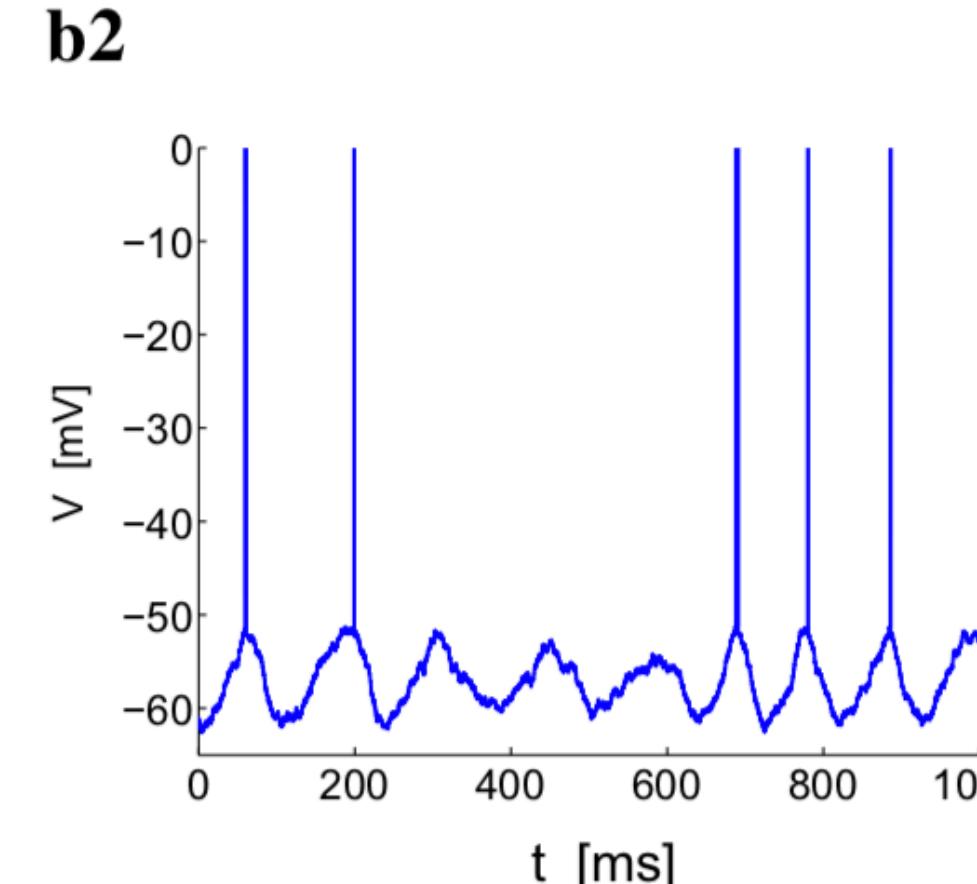
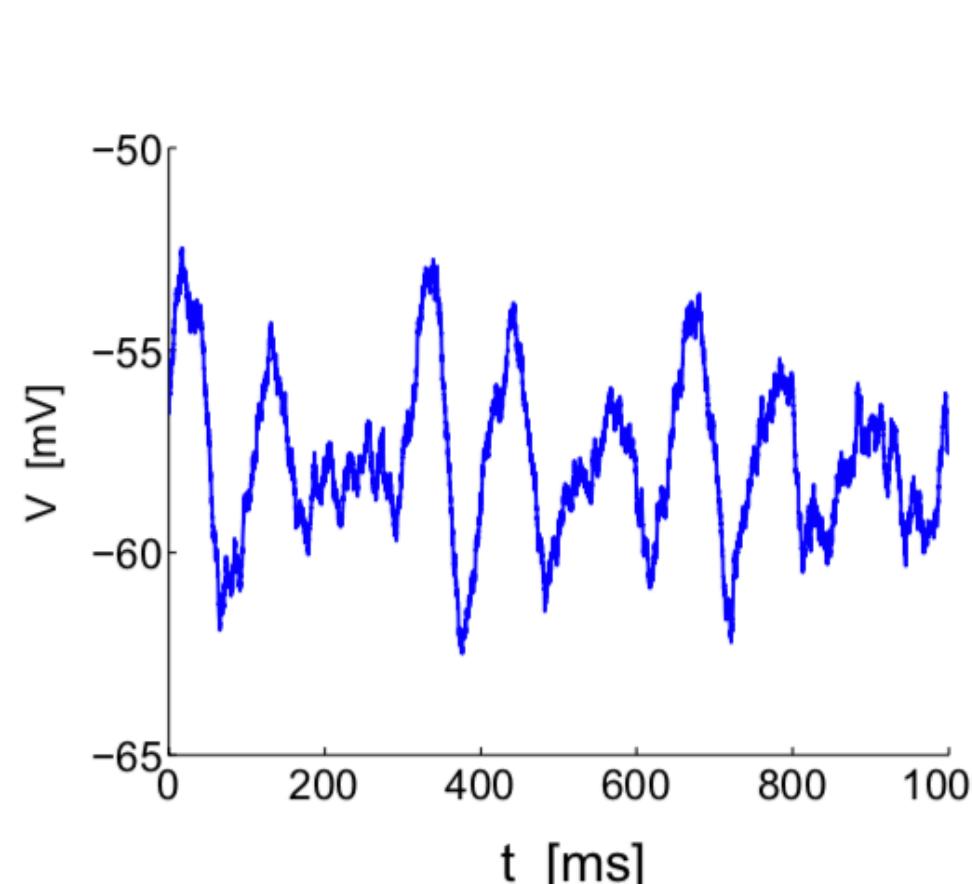
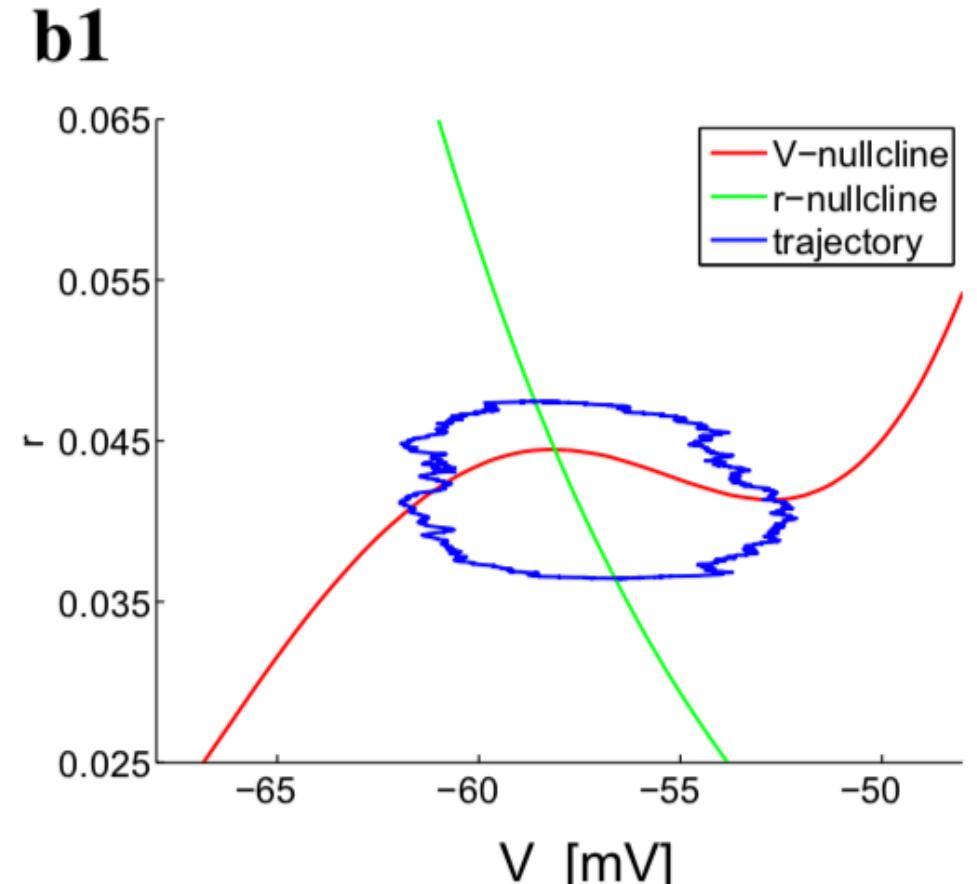
**Model 1**



Differences:

- Geometry: parabolic- and cubic-like
- Generation of STOs in the parabolic- and cubic-like
- Transition from STOs to spikes

**Model 2**

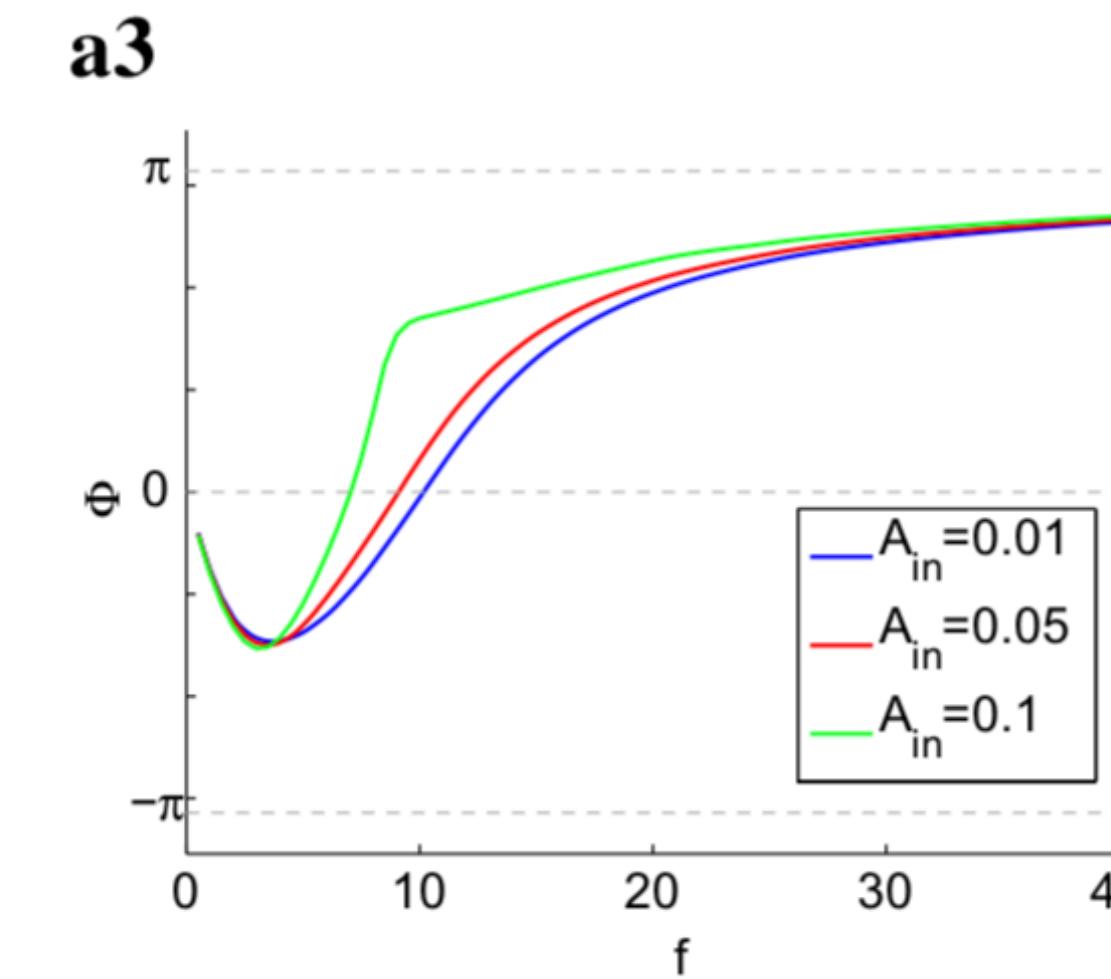
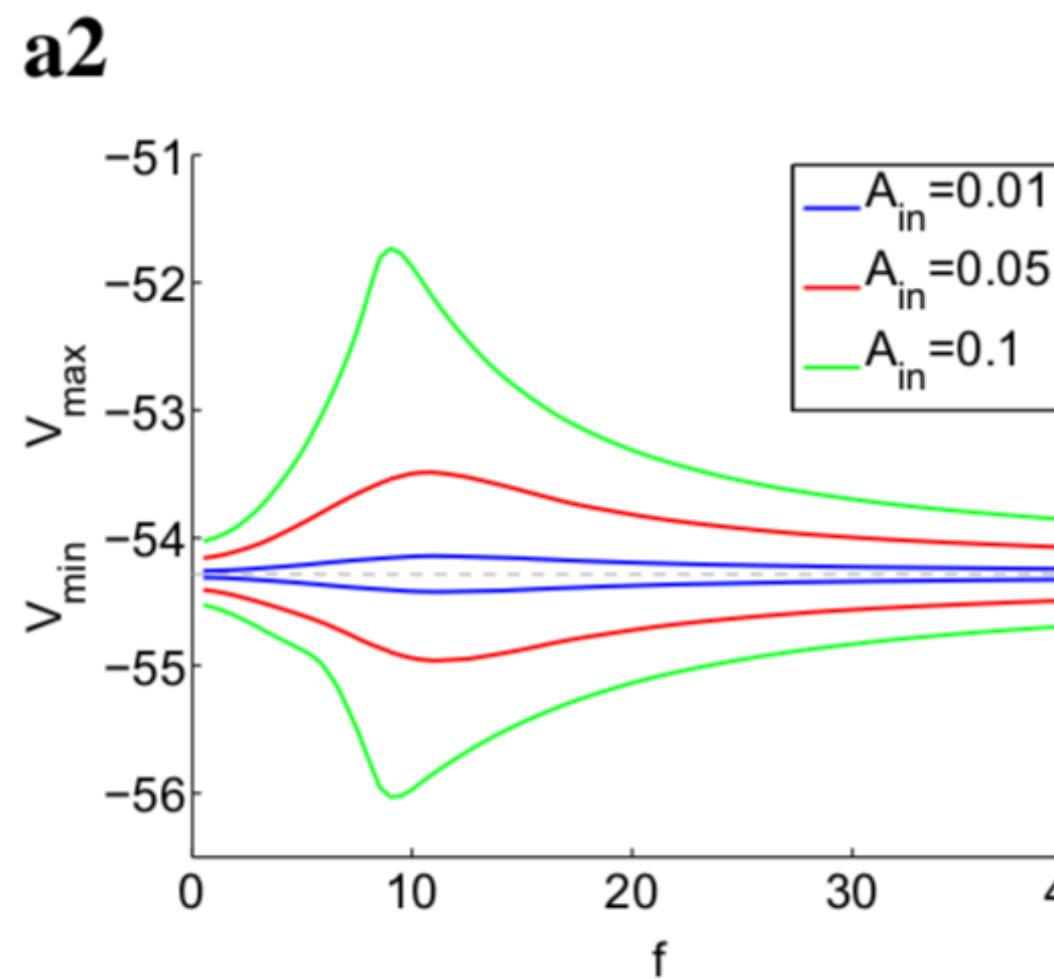
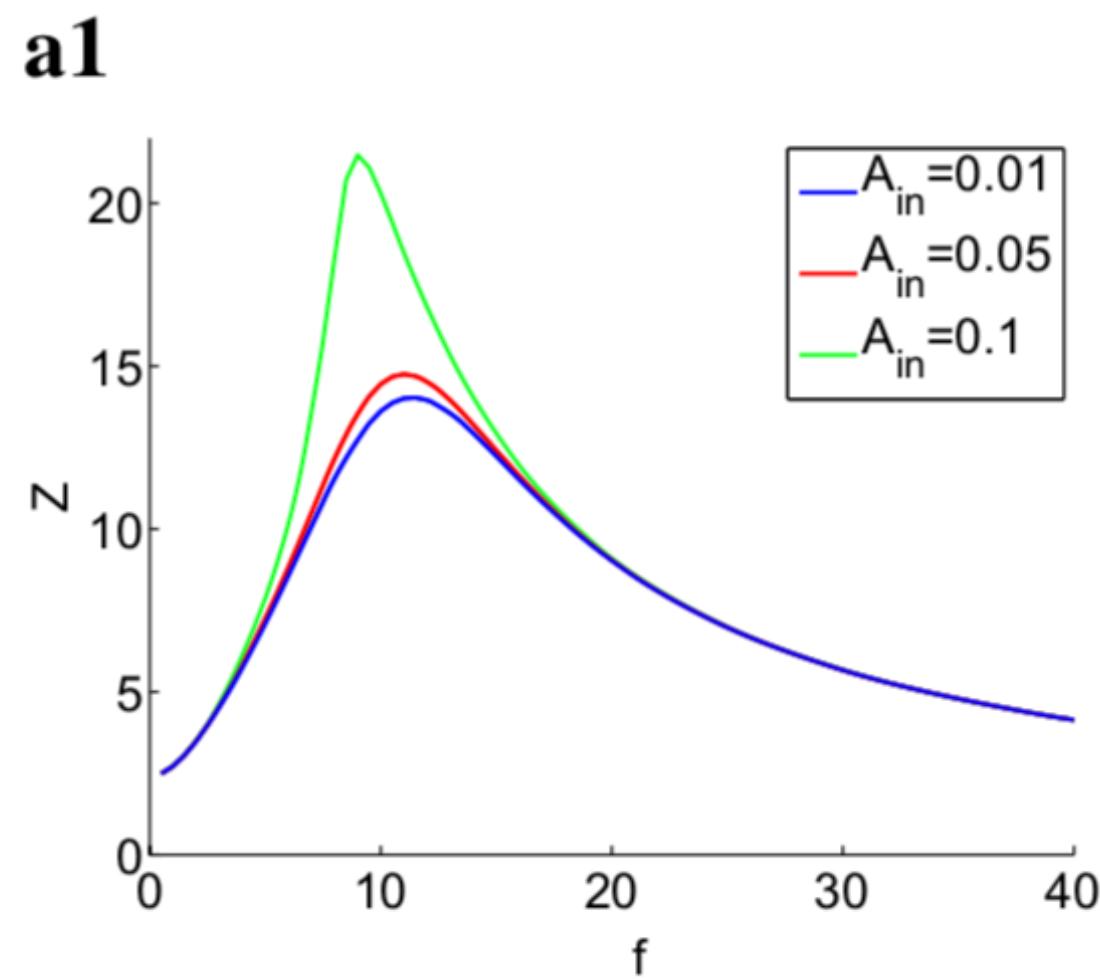


→ **model 1** generates damped STOs but not persistent  
(unless noise is present).

→ **model 2** generates persistent STOs  
No mechanism for the onset of spikes.

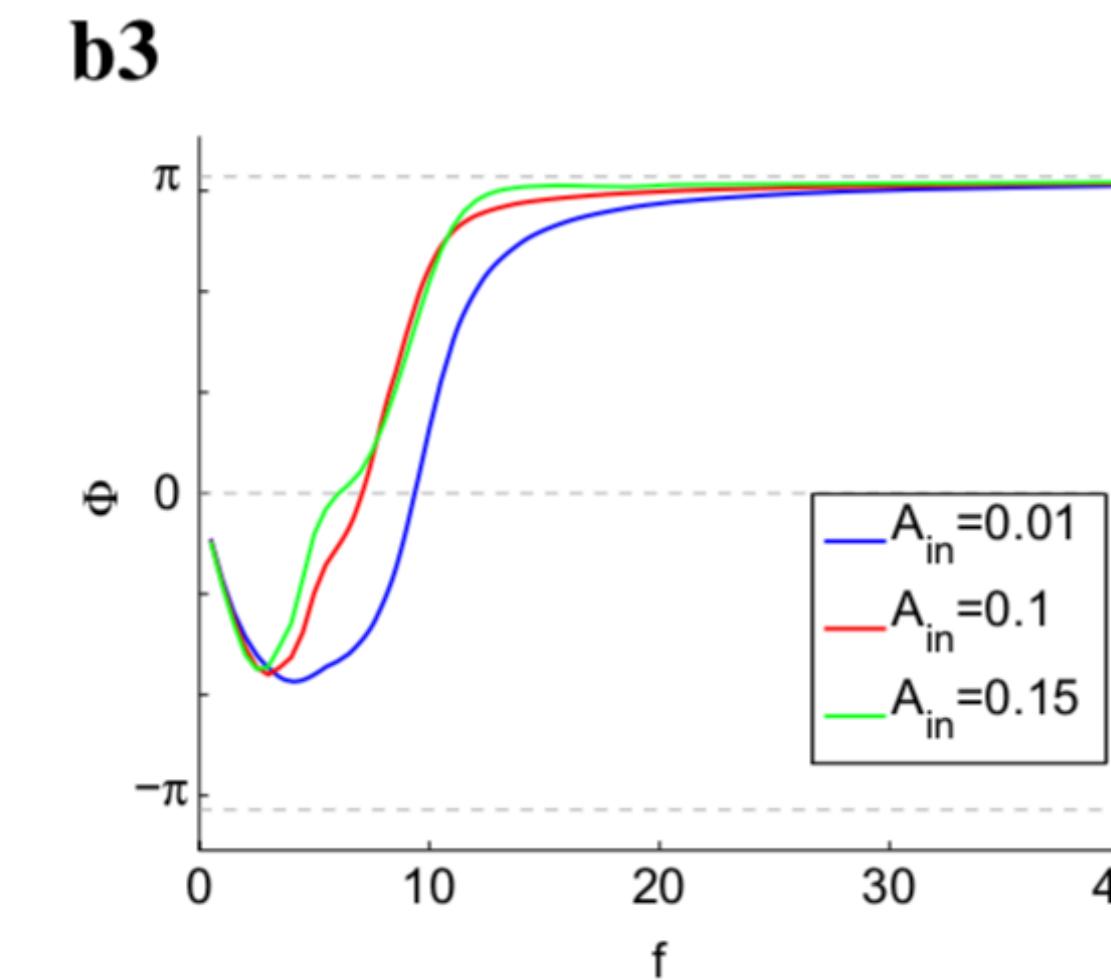
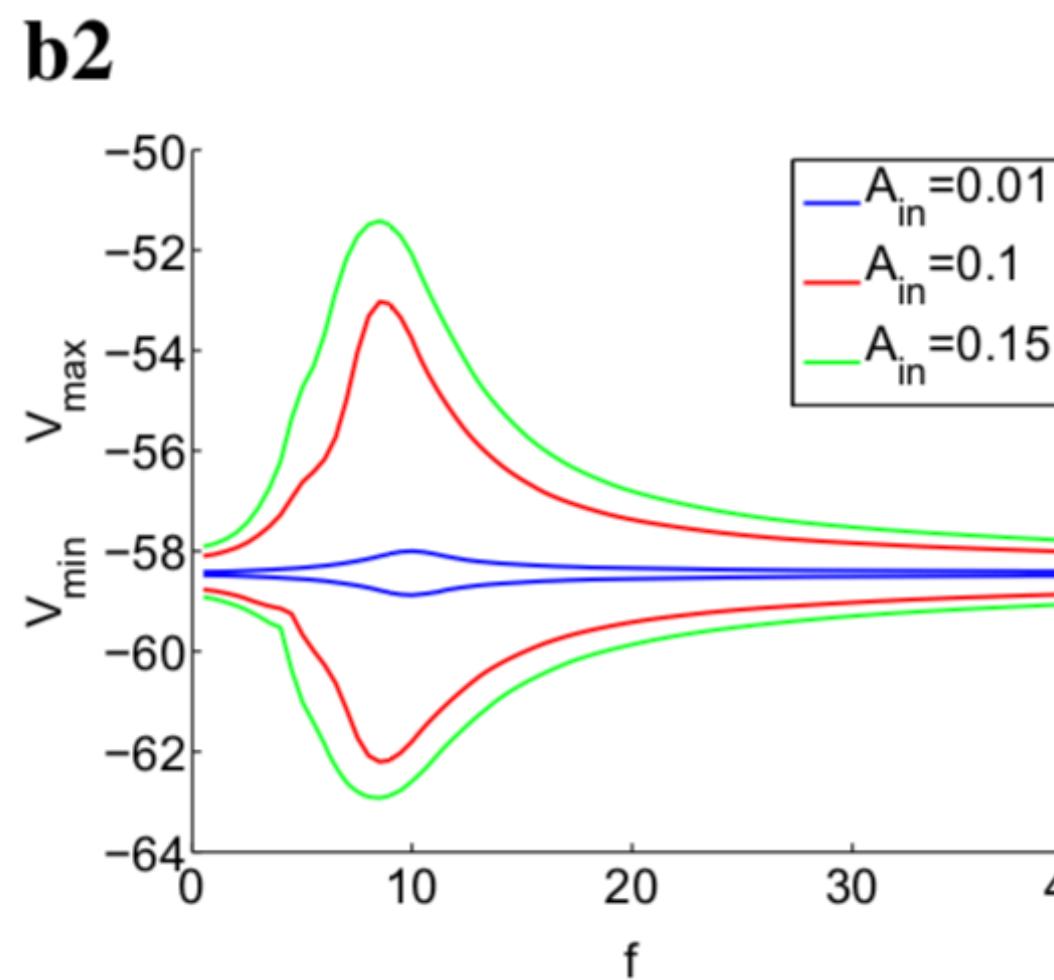
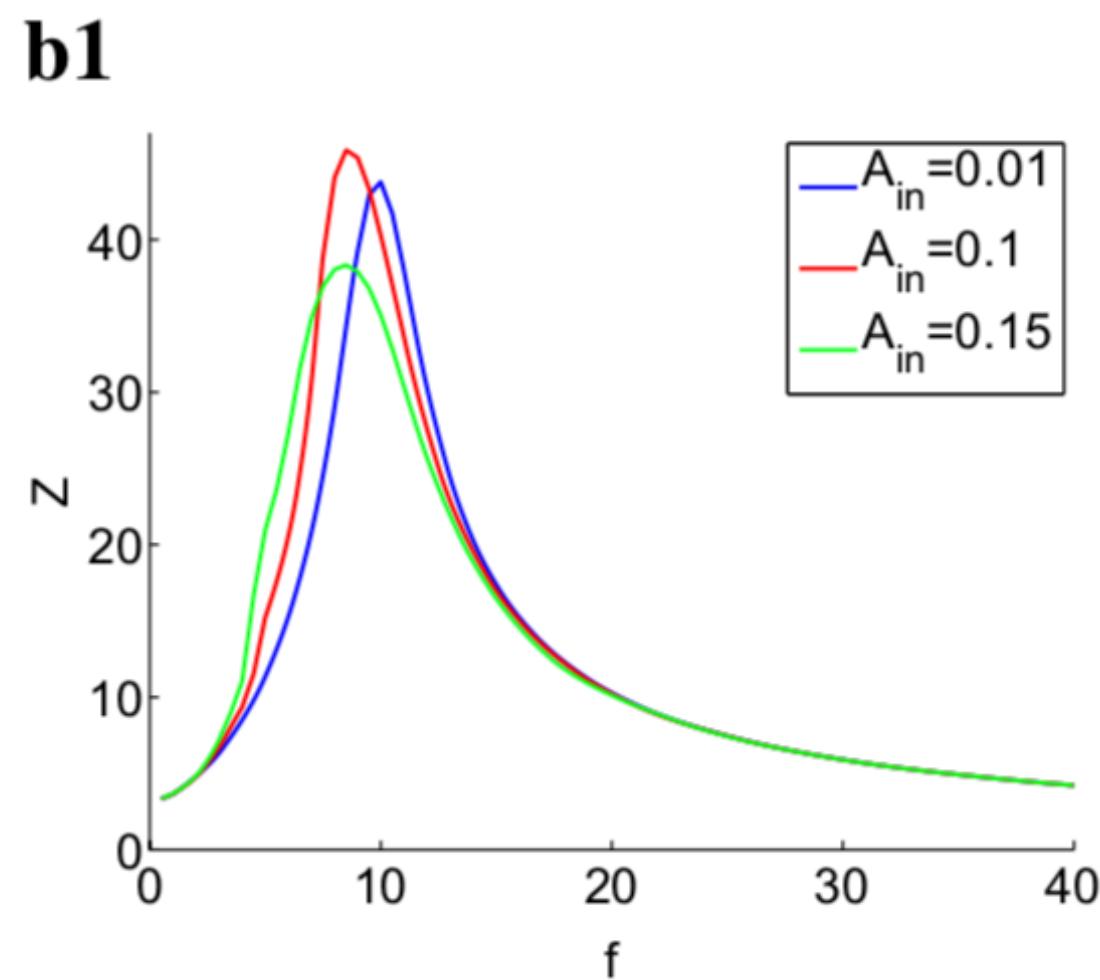
# From subthreshold to spikes

Model 1 (parabolic)



Both models exhibit **resonance** and **phasonance** in theta (4–12 Hz).

Model 2 (cubic)



# How to access suprathreshold resonance

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- spike-frequency ( $f_{\text{spk}}$ ) response to oscillatory input currents;
- spike-phase ( $\phi_{\text{spk}}$ ) response to oscillatory input currents.

- spike-frequency ( $f_{\text{spk}}$ ) response to oscillatory input currents;

### *Evoked spiking resonance*

spikes generated for **intermediate** (resonant) input **frequency** band  $\Delta f_{\text{res,ev}}$

### *Output spiking resonance*

output frequency belongs to an intermediate (resonant) frequency band  $\Delta f_{\text{res,out}}$ ,  
**regardless of the input frequency** that generated the response

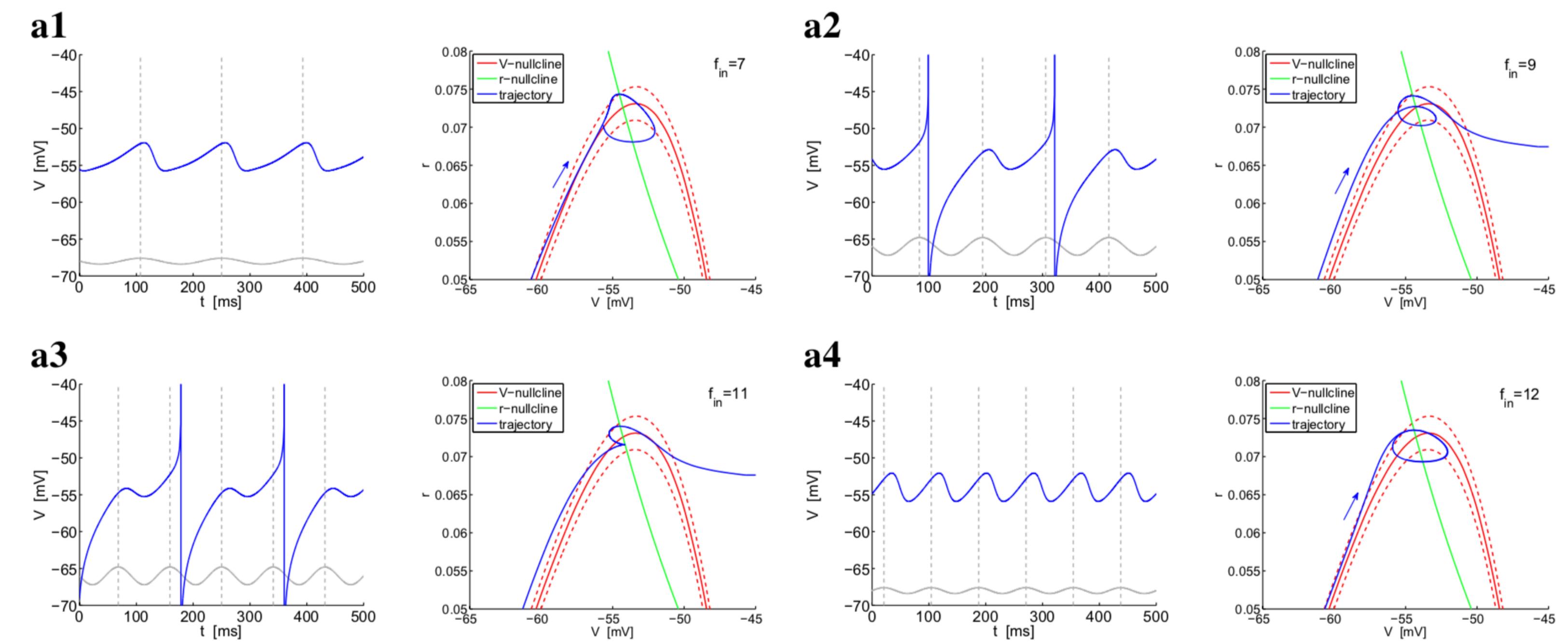
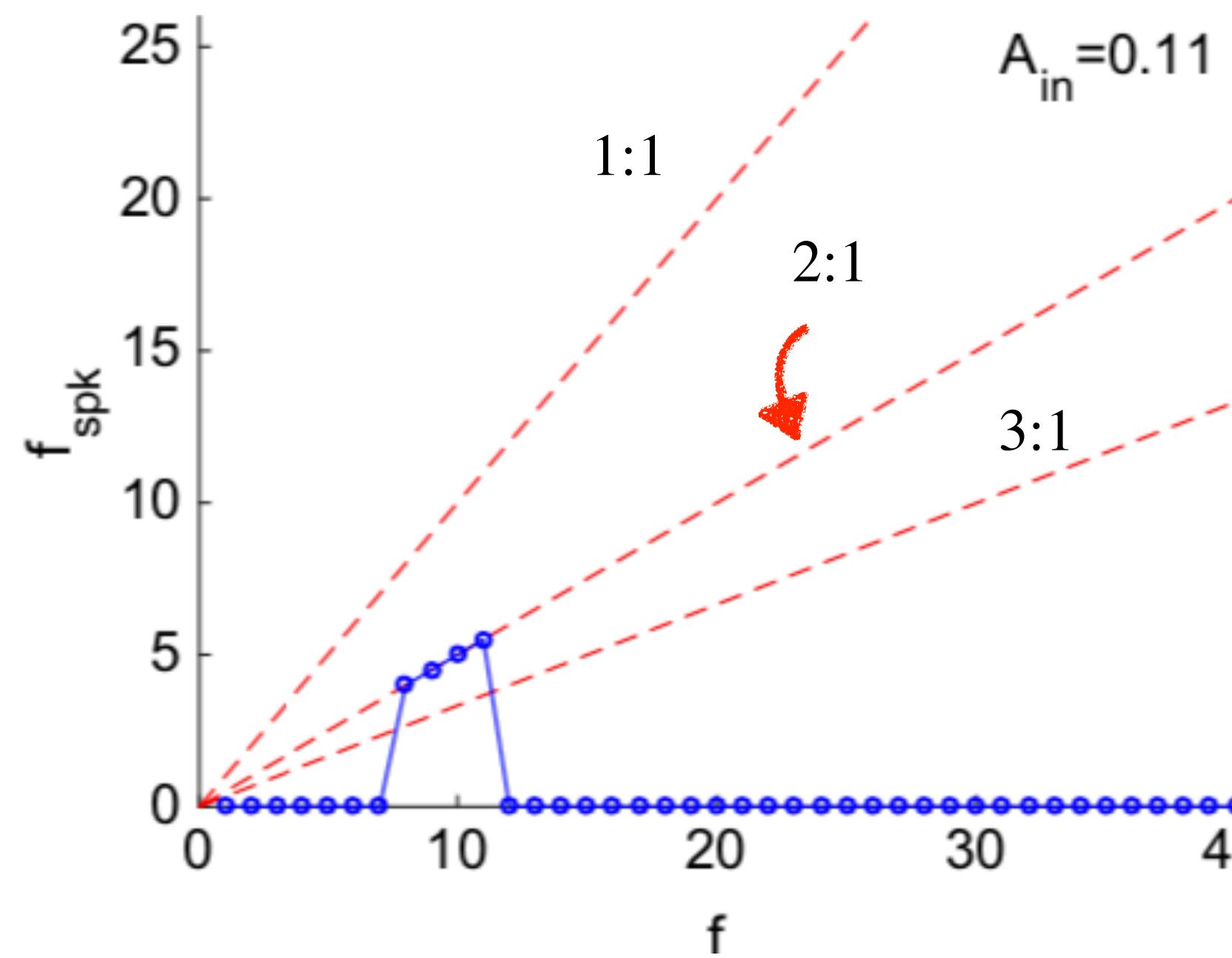
- spike-phase ( $\phi_{\text{spk}}$ ) response to oscillatory input currents.

### *Spiking phasonance*

Zero spiking phase-shift (spiking phase)  $\phi_{\text{spk}}$  between the **output spike** and the **input peak**

# Model 1 - low amplitude regime

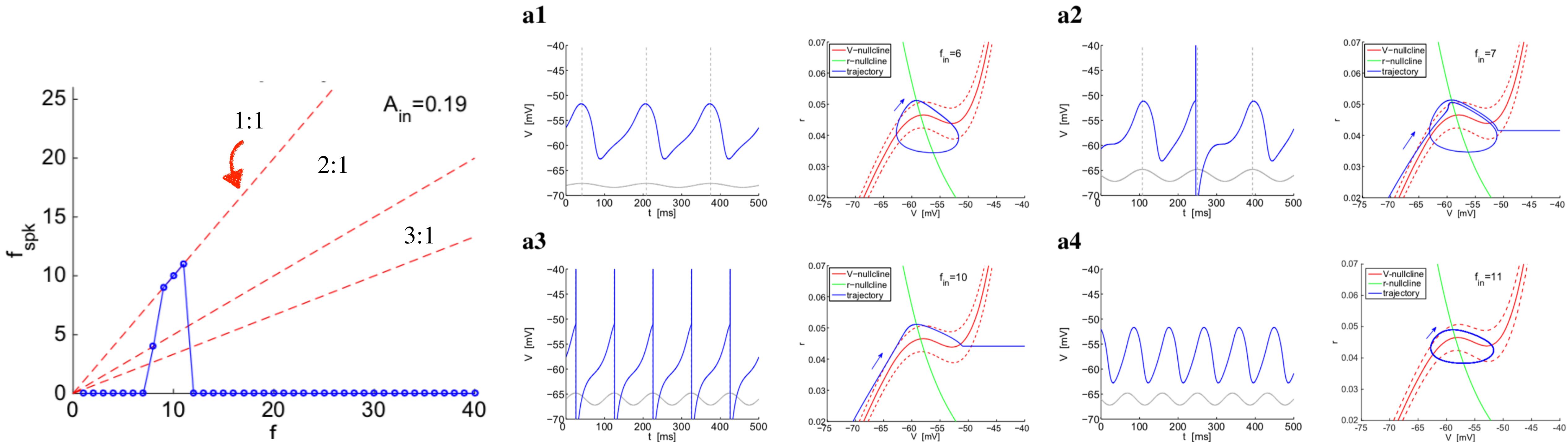
- Subthreshold resonance is communicated to the suprathreshold regime to produce both **evoked** and **output** spiking resonance



Rotstein, *J Comput Neurosci* (2017) 43:243–271

# Model 2 - low amplitude regime

- Subthreshold resonance is **also** communicated to the suprathreshold regime to produce both **evoked** and **output** spiking resonance

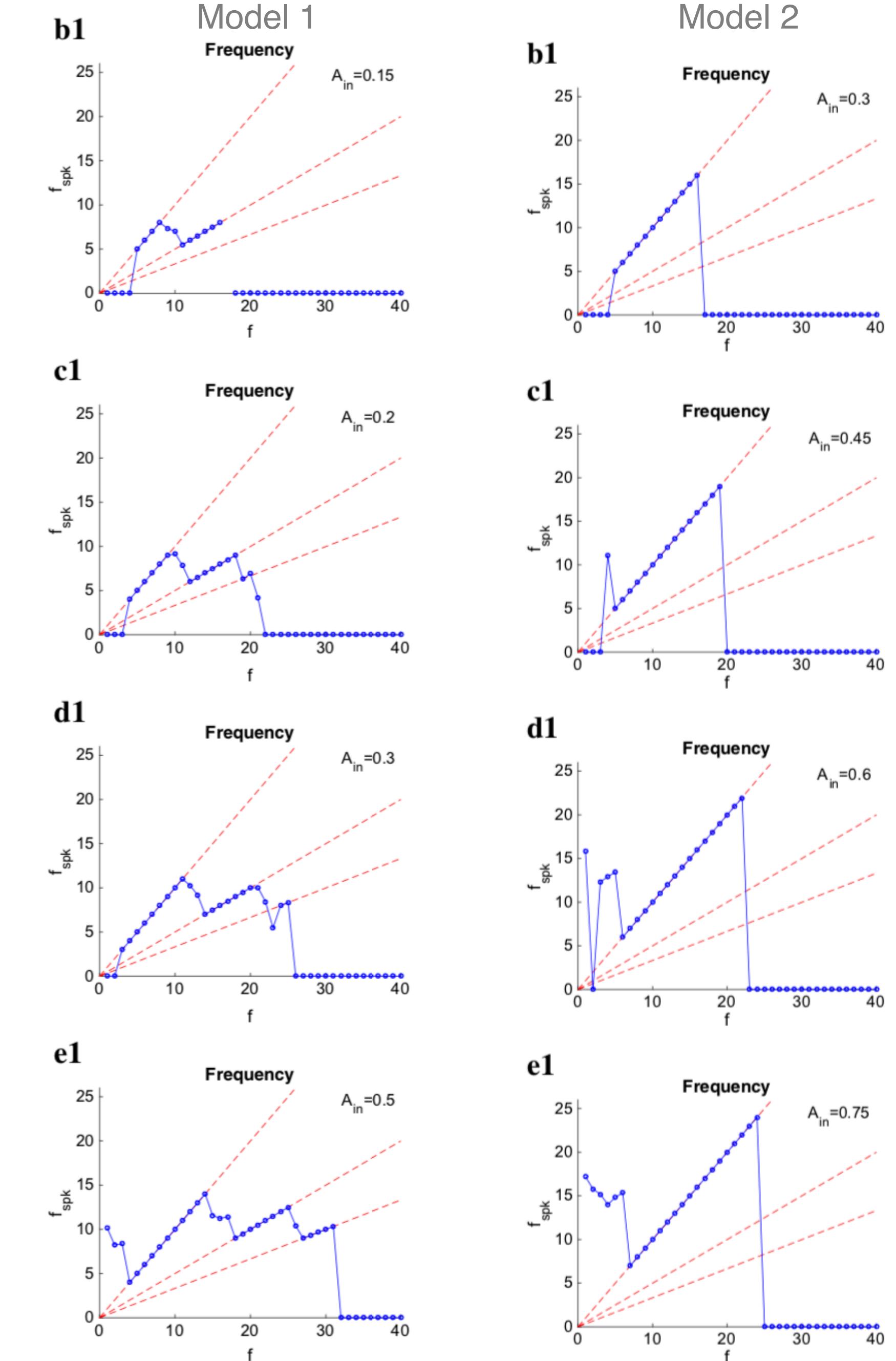


Rotstein, *J Comput Neurosci* (2017) 43:243–271

Evoked theta spiking resonance vanishes for  
larger amplitudes  
-> low-pass filters

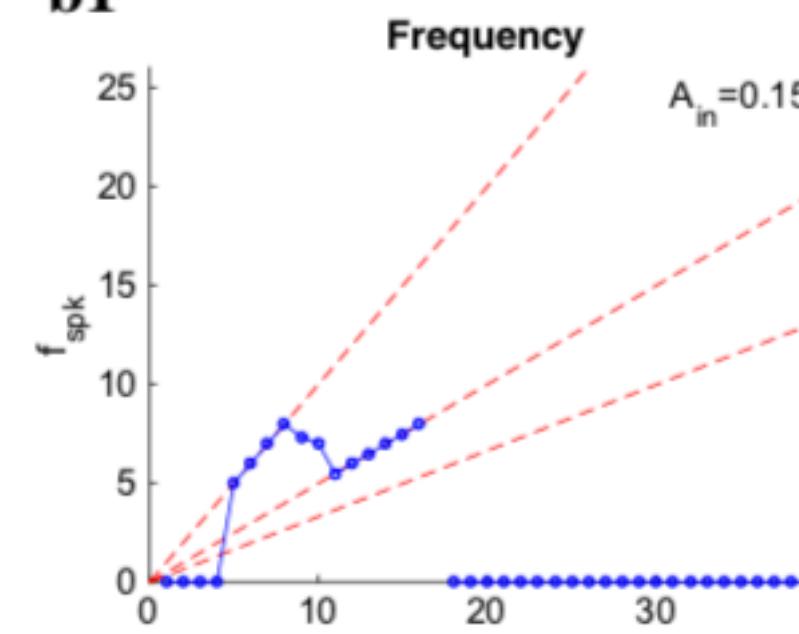
- evoked spiking resonance for low amplitude due to **subthreshold upper envelope**
- evoked spiking **low-pass filter** for higher amplitudes

Increasing  
Amplitude

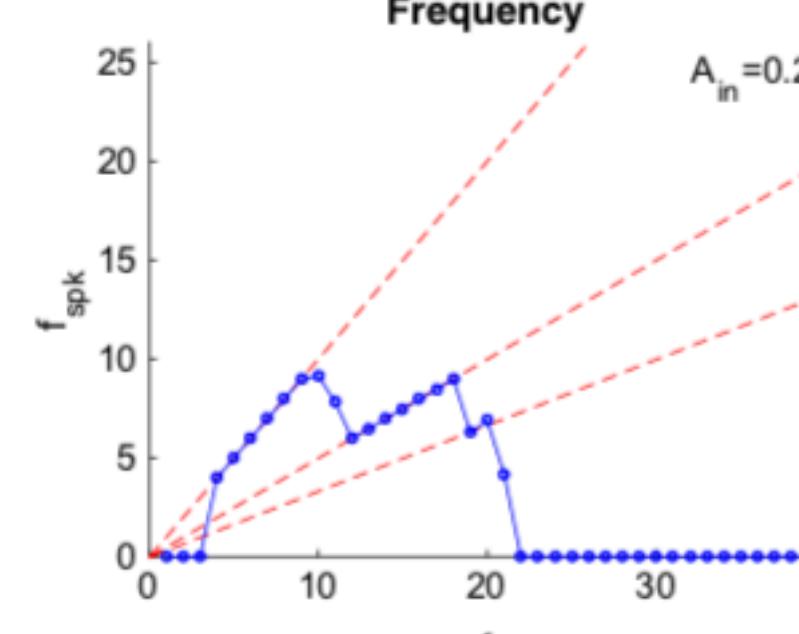


# Model 1 - intermediate amplitude regime

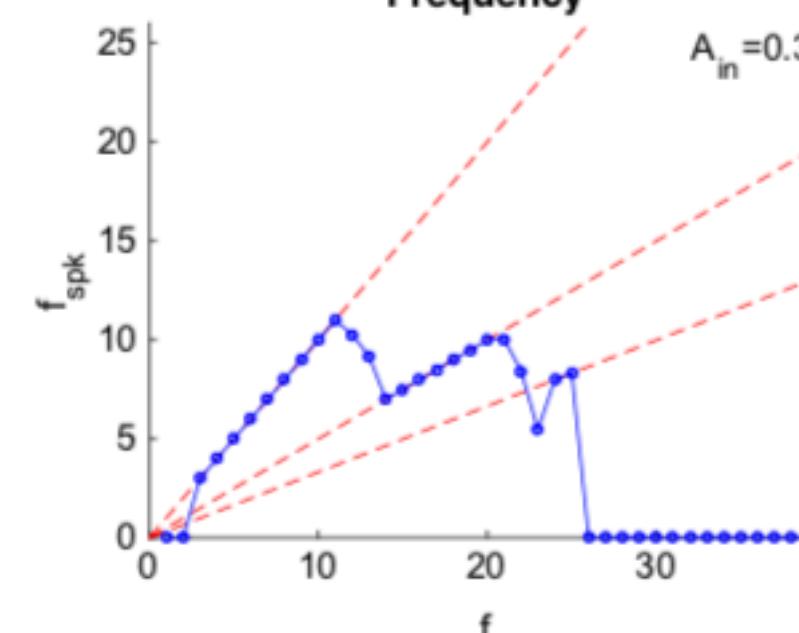
b1



c1



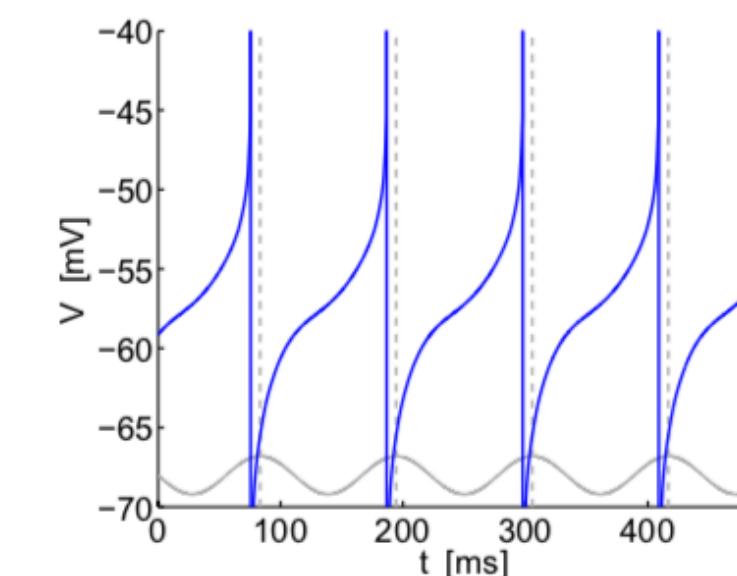
d1



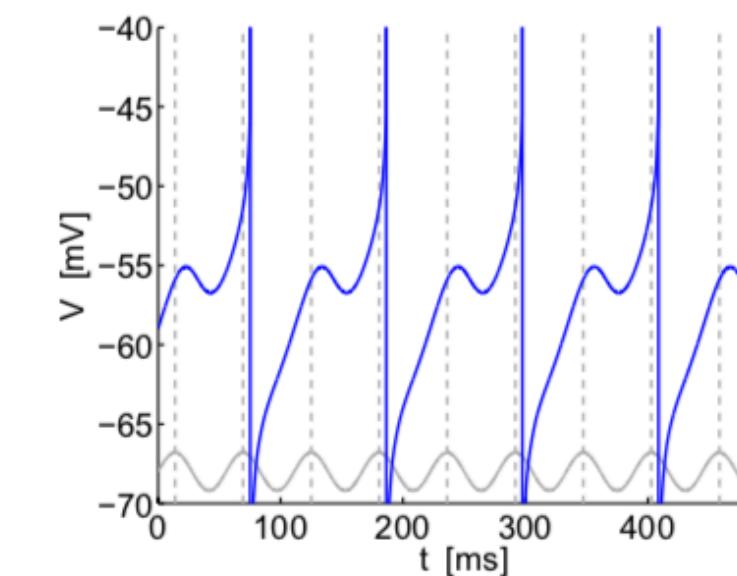
Increasing Amplitude  
↓

- theta output resonance for intermediate values of  $A_{\text{in}}$

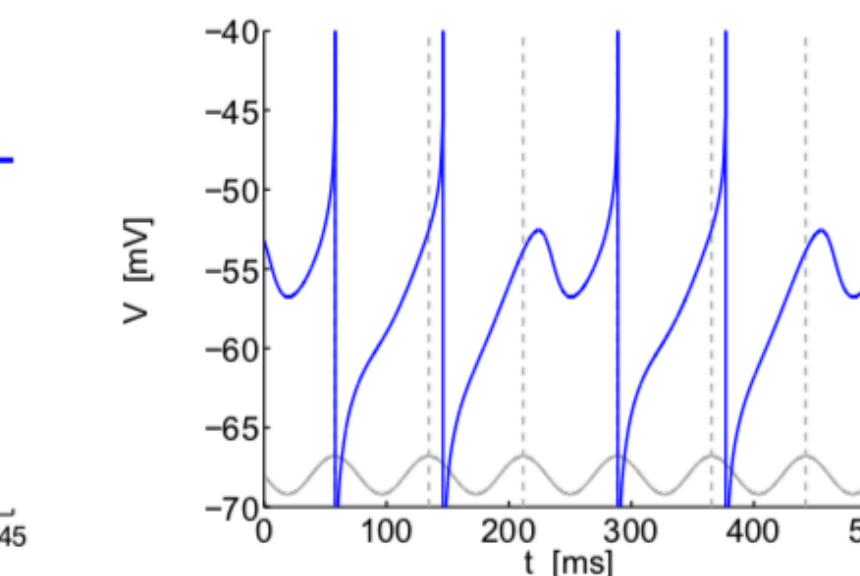
b1



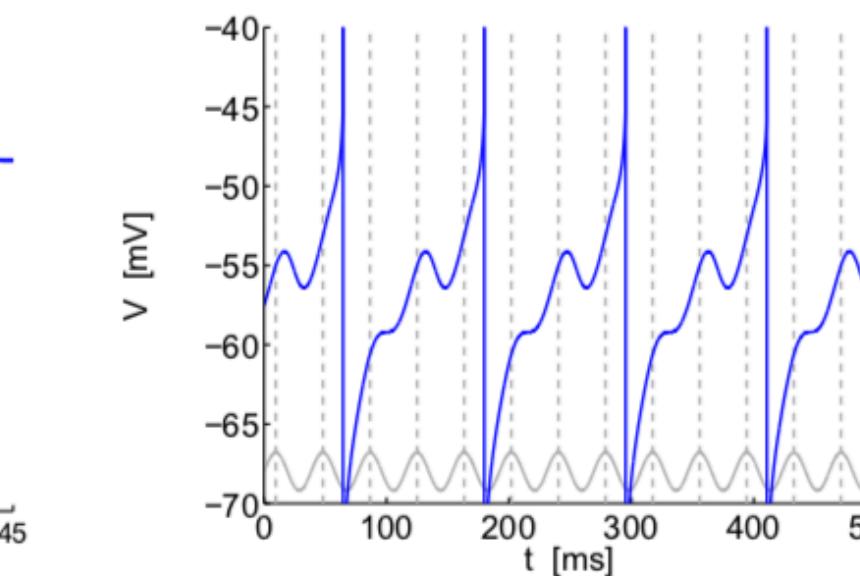
b3



b2

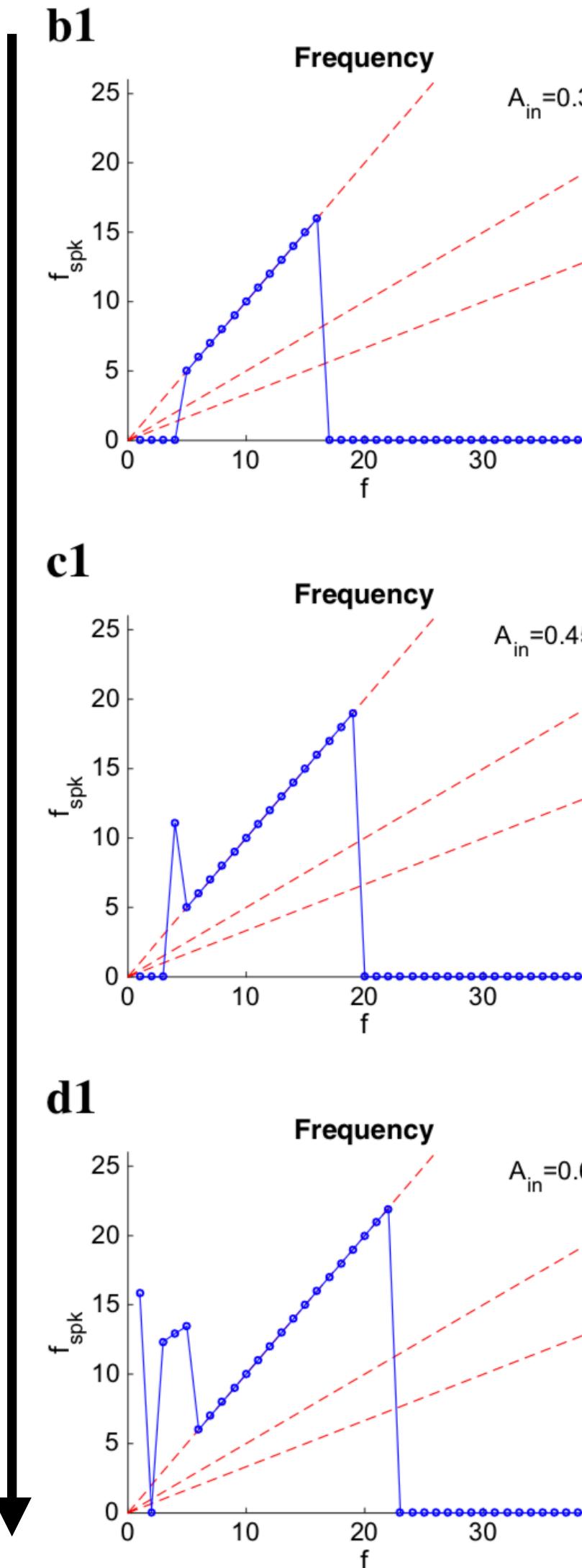


b4

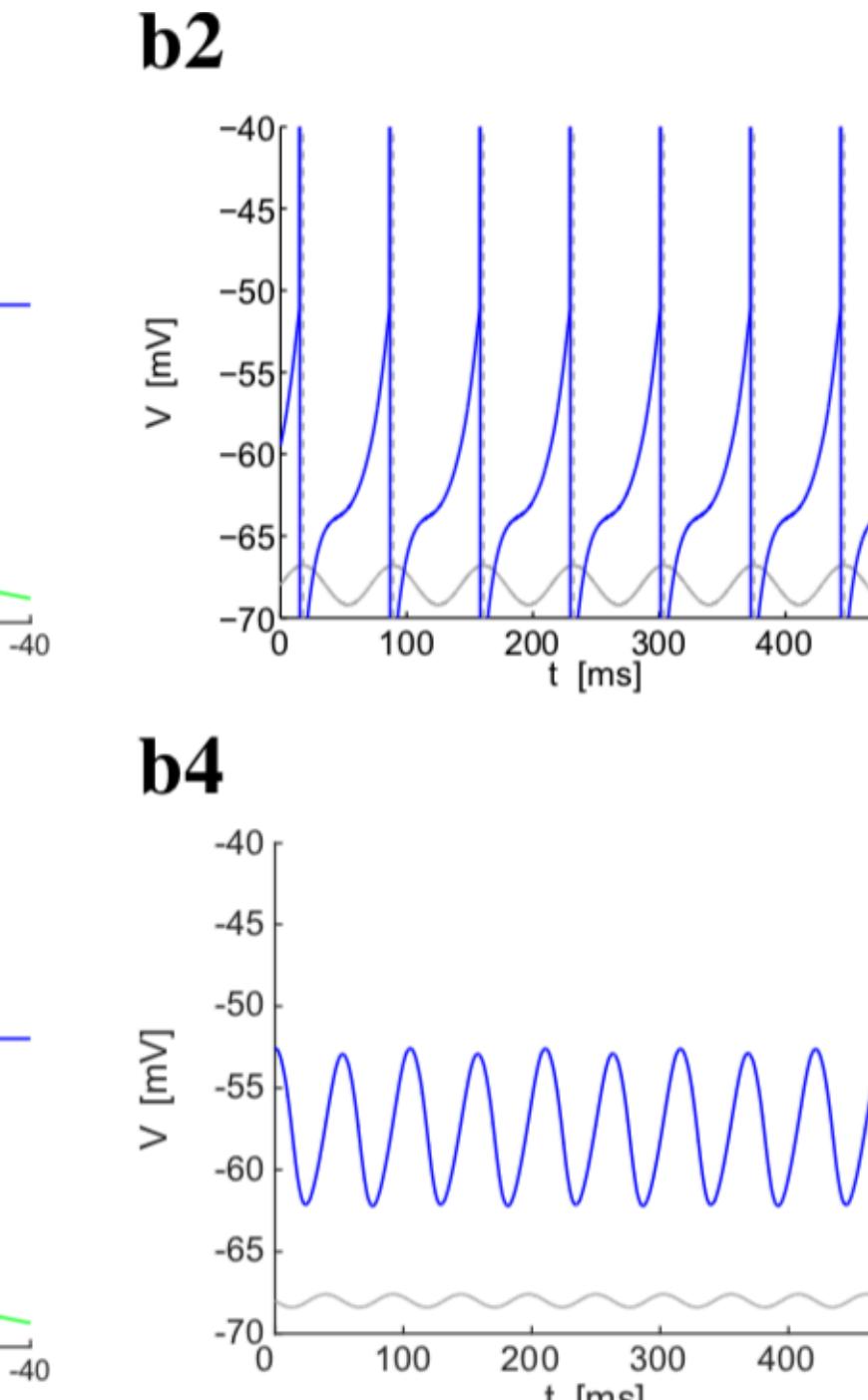
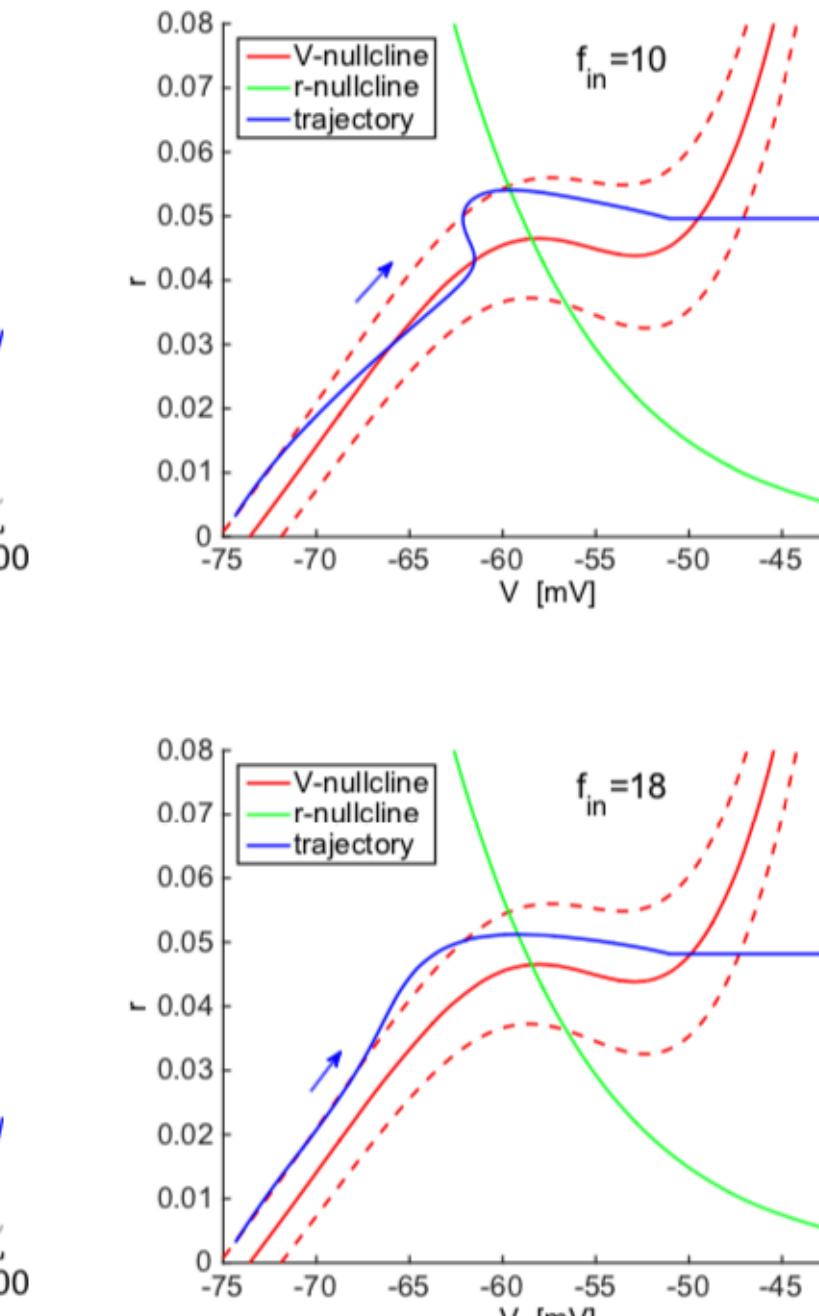
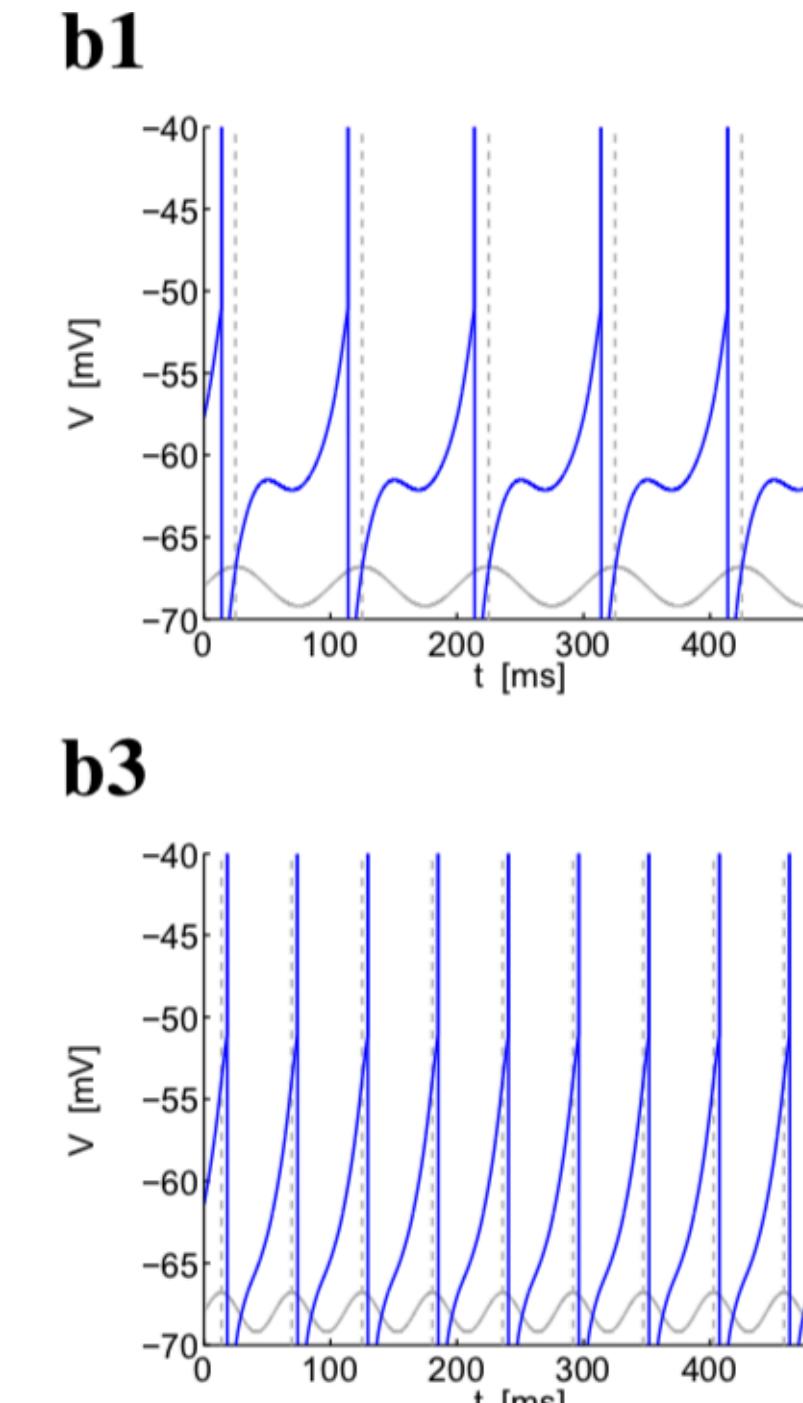


- cycle skipping mechanisms allows patterns 2:1 and 3:1 in addition to the 1:1

# Model 2 - intermediate amplitude regime



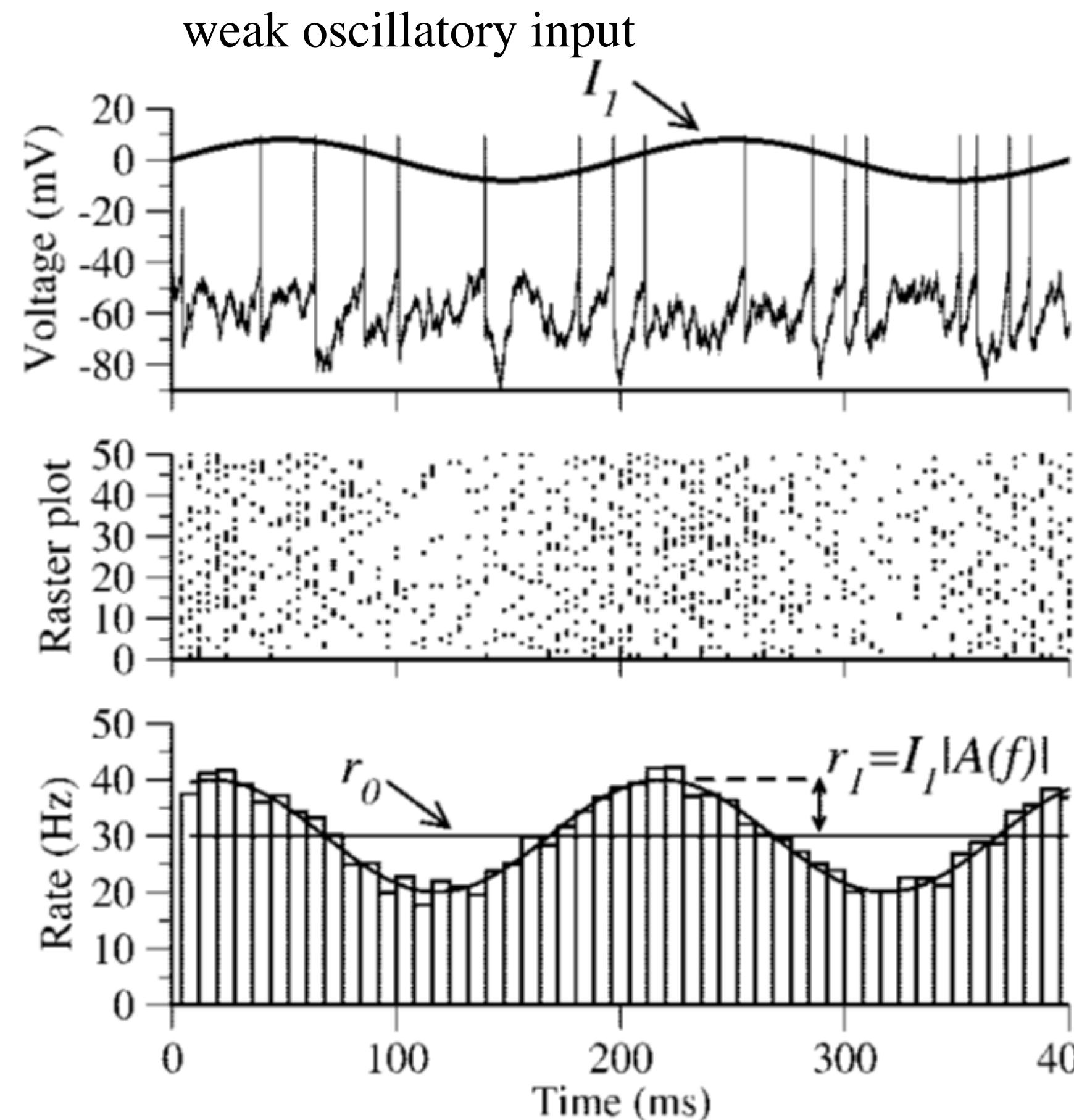
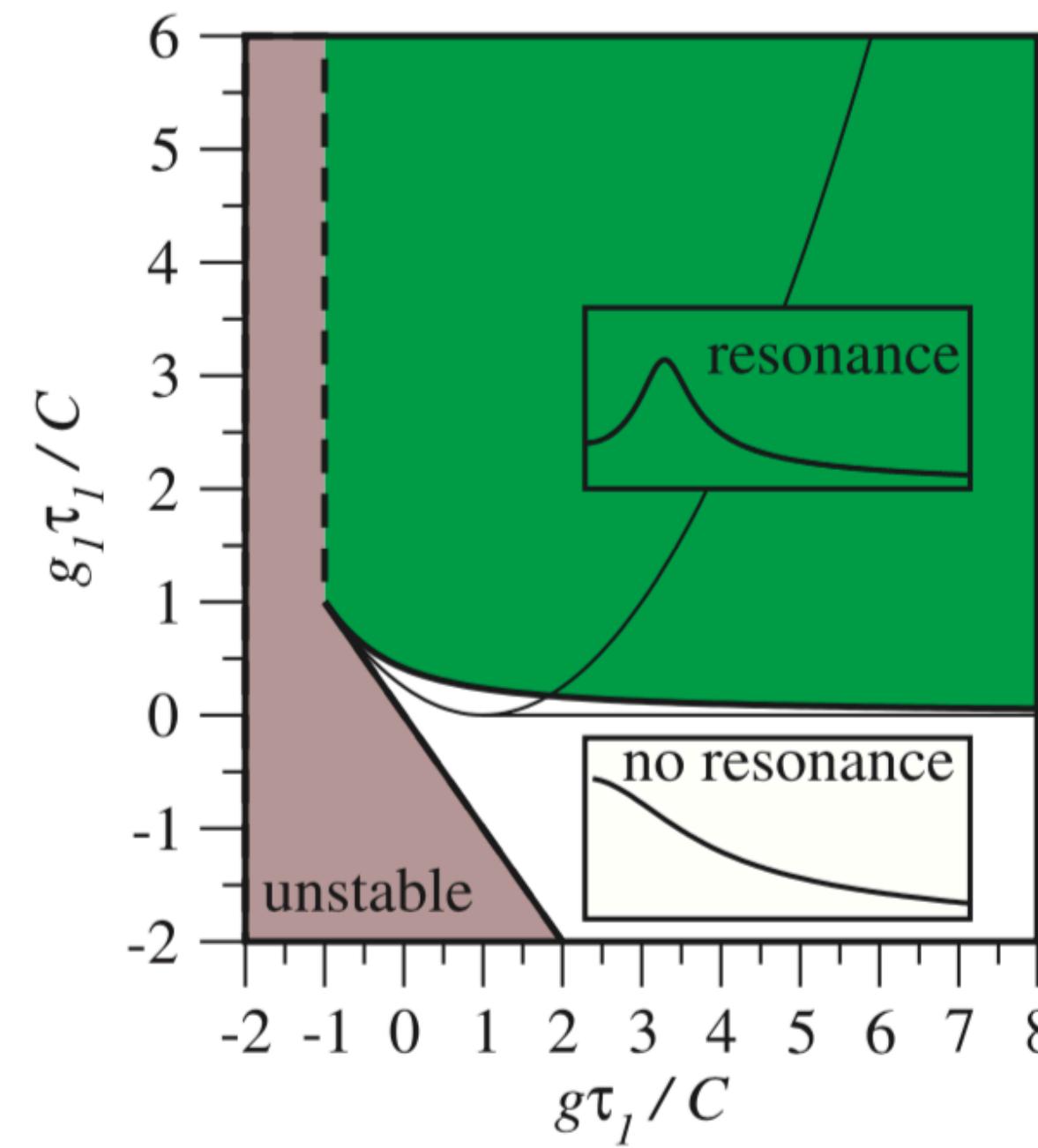
- Broad-band output response for intermediate amplitudes



- No cycle skipping mechanisms, patterns continue 1:1 even for higher frequencies

$$C \frac{dv}{dt} = -gv - g_1 w + I_{\text{app}}(t)$$

$$\tau_1 \frac{dw}{dt} = v - w$$



Richardson et al., *J Neurophysiol* (2003)  
89:2538–2554

Two distinct and independent frequency scales:

**Subthreshold resonant frequency  $f_R$**

subthreshold dynamics of the membrane potential

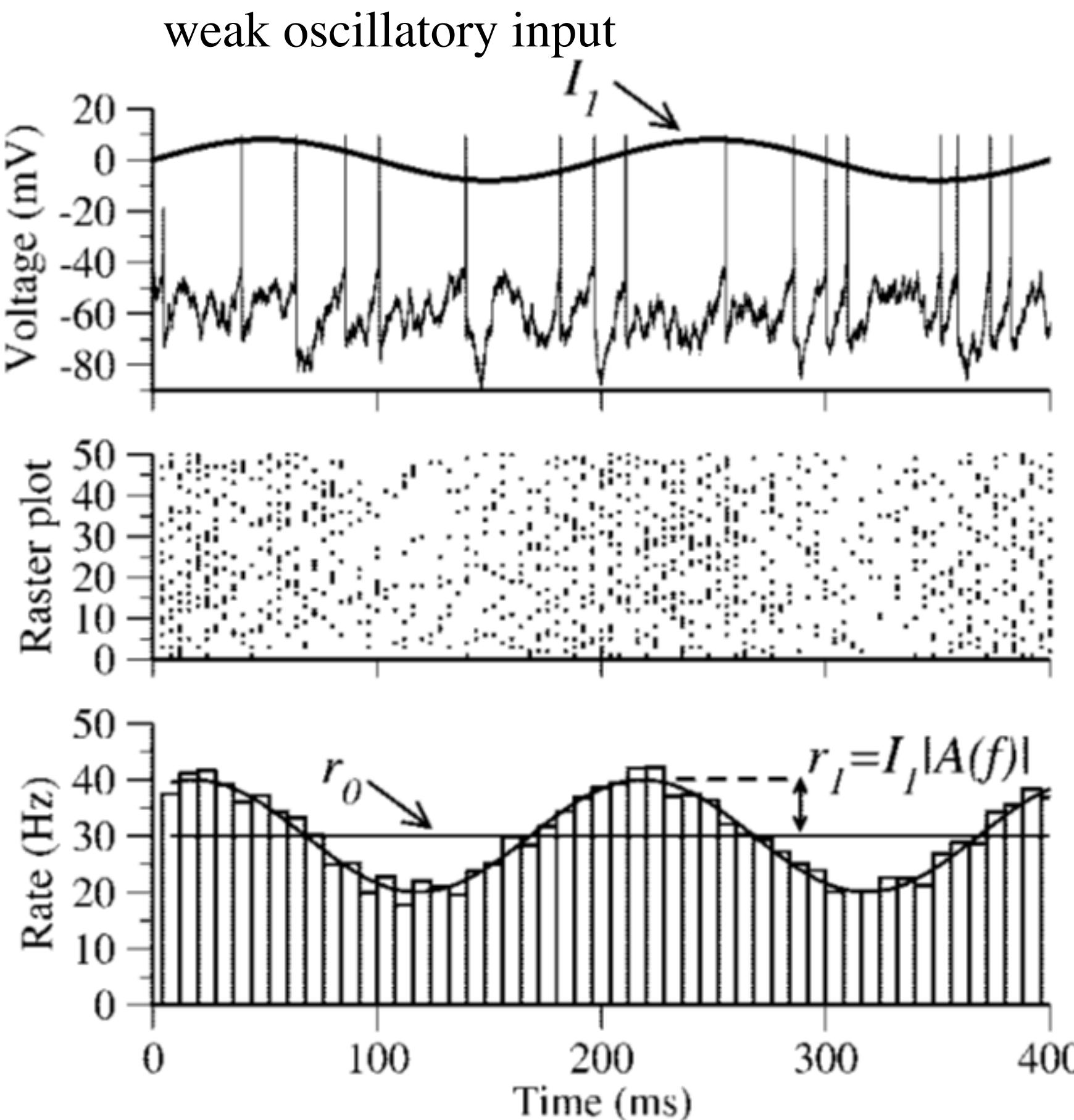
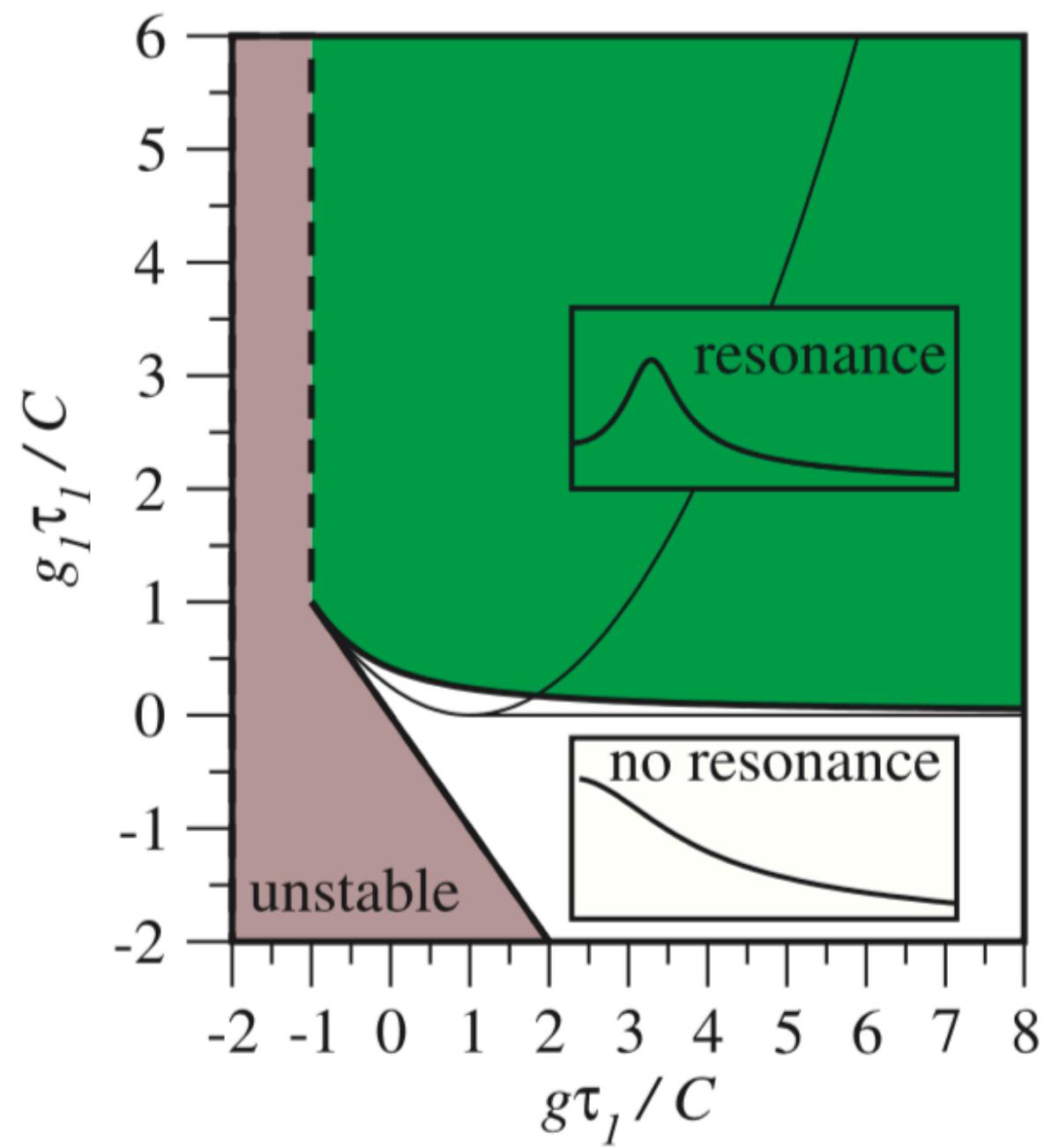
**Background firing frequency  $r_0$**

externally applied noisy current

## Defining in terms of the population population

$$C \frac{dv}{dt} = -gv - g_1 w + I_{\text{app}}(t)$$

$$\tau_1 \frac{dw}{dt} = v - w$$



Richardson et al., *J Neurophysiol* (2003)  
89:2538–2554

signal gain

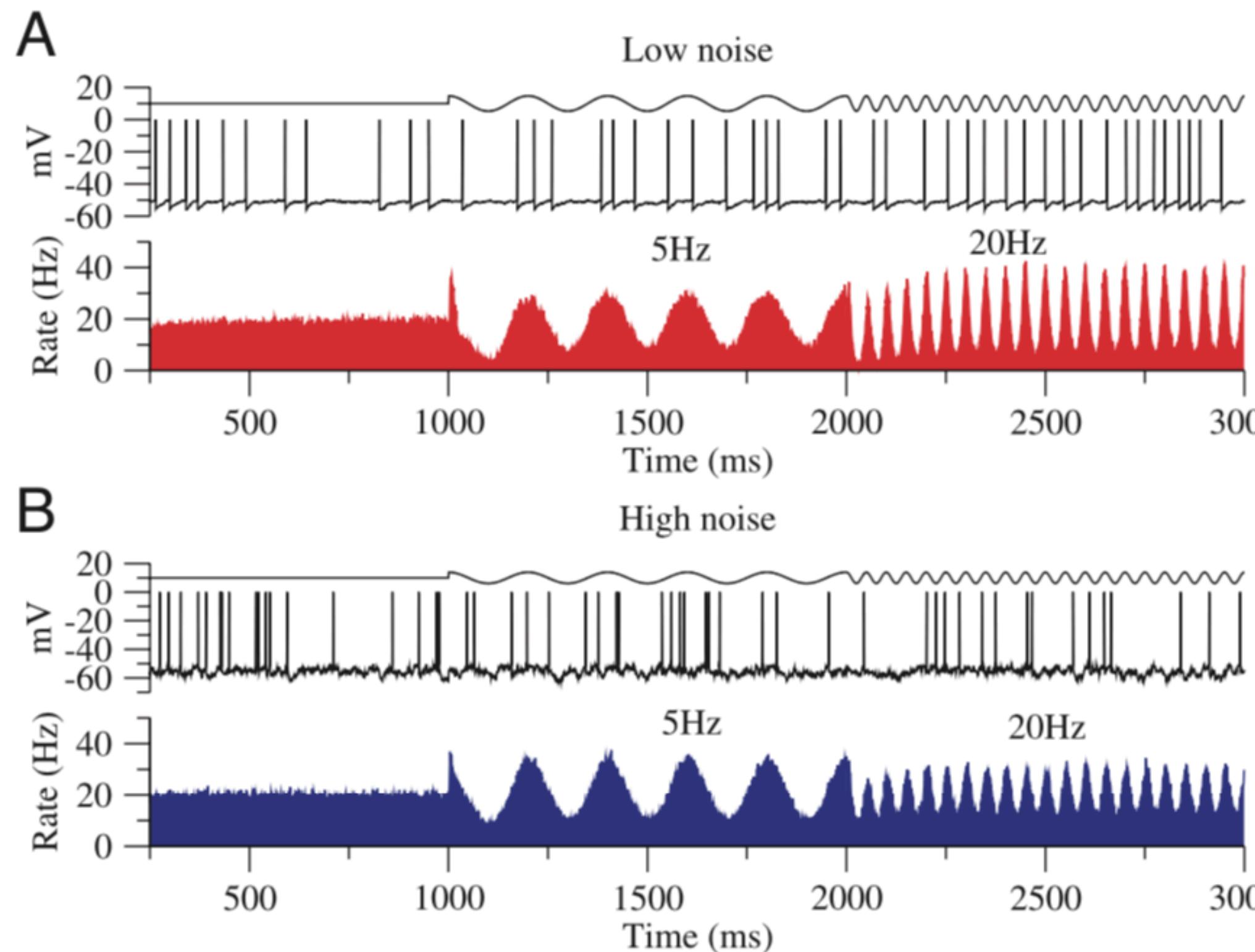
$$|A(f)| = r_1(f)/I_1$$

Note similarity  
with impedance

$$|Z(f)| = V_1(f)/I_1$$

## Effect of noise (high firing rate $r_0 > f_R$ )

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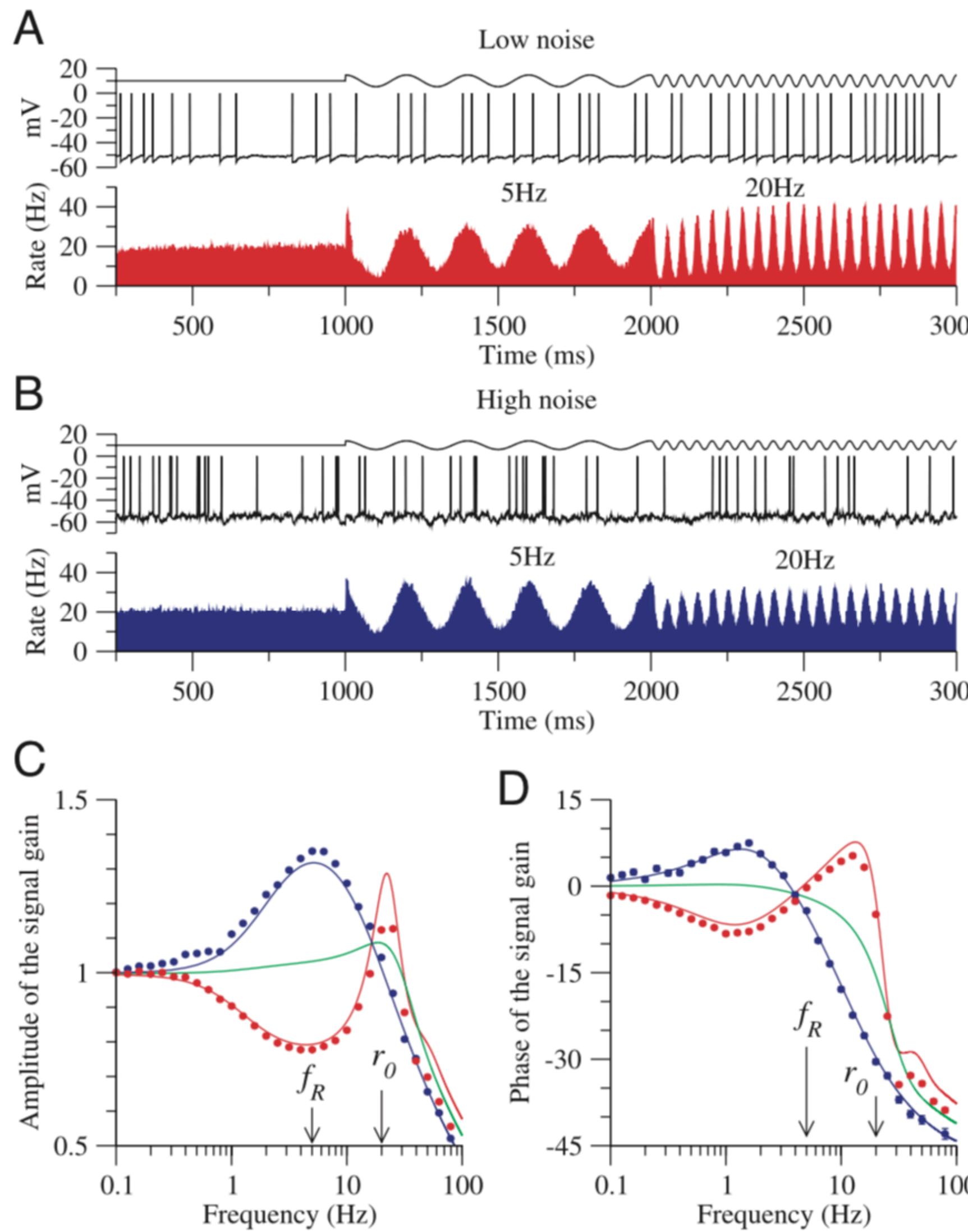


Two distinct modes of behavior

- regular firing (*low noise*);
- irregular firing (*high noise*).

Richardson et al., *J Neurophysiol* (2003) 89:2538–2554

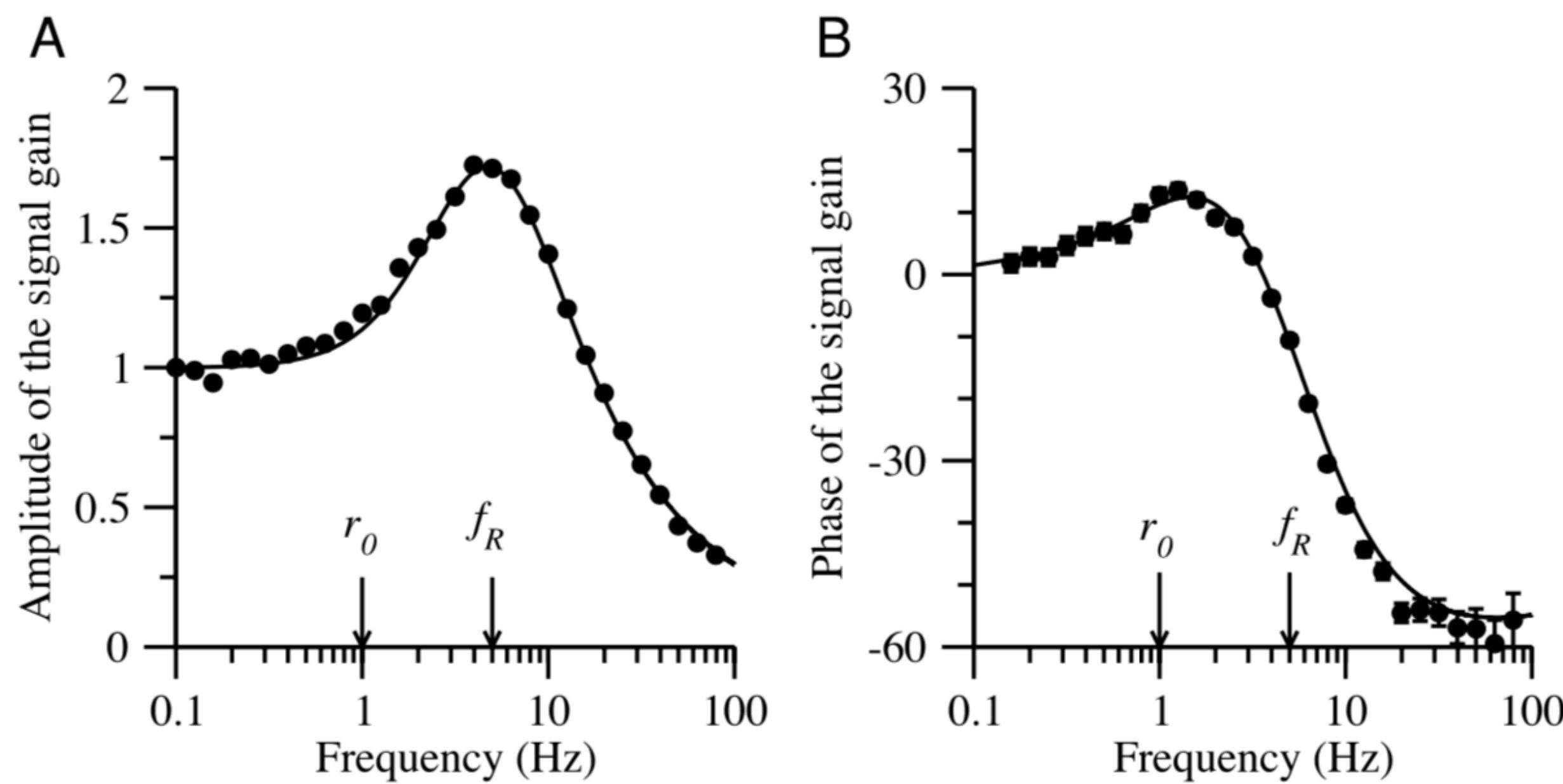
## Effect of noise (high firing rate $r_0 > f_R$ )



Two distinct modes of behavior

- regular firing (*low noise*);
- irregular firing (*high noise*).

Richardson et al., *J Neurophysiol* (2003) 89:2538–2554



Richardson et al., *J Neurophysiol* (2003) 89:2538–2554

For  $r_0 < f_R$ , high noise is necessary to achieve lower frequencies

(type II neuron starts firing at finite frequency)

inter-spike interval is long:  
neuron has time to explore subthreshold regime and begin to “resonate” before firing.

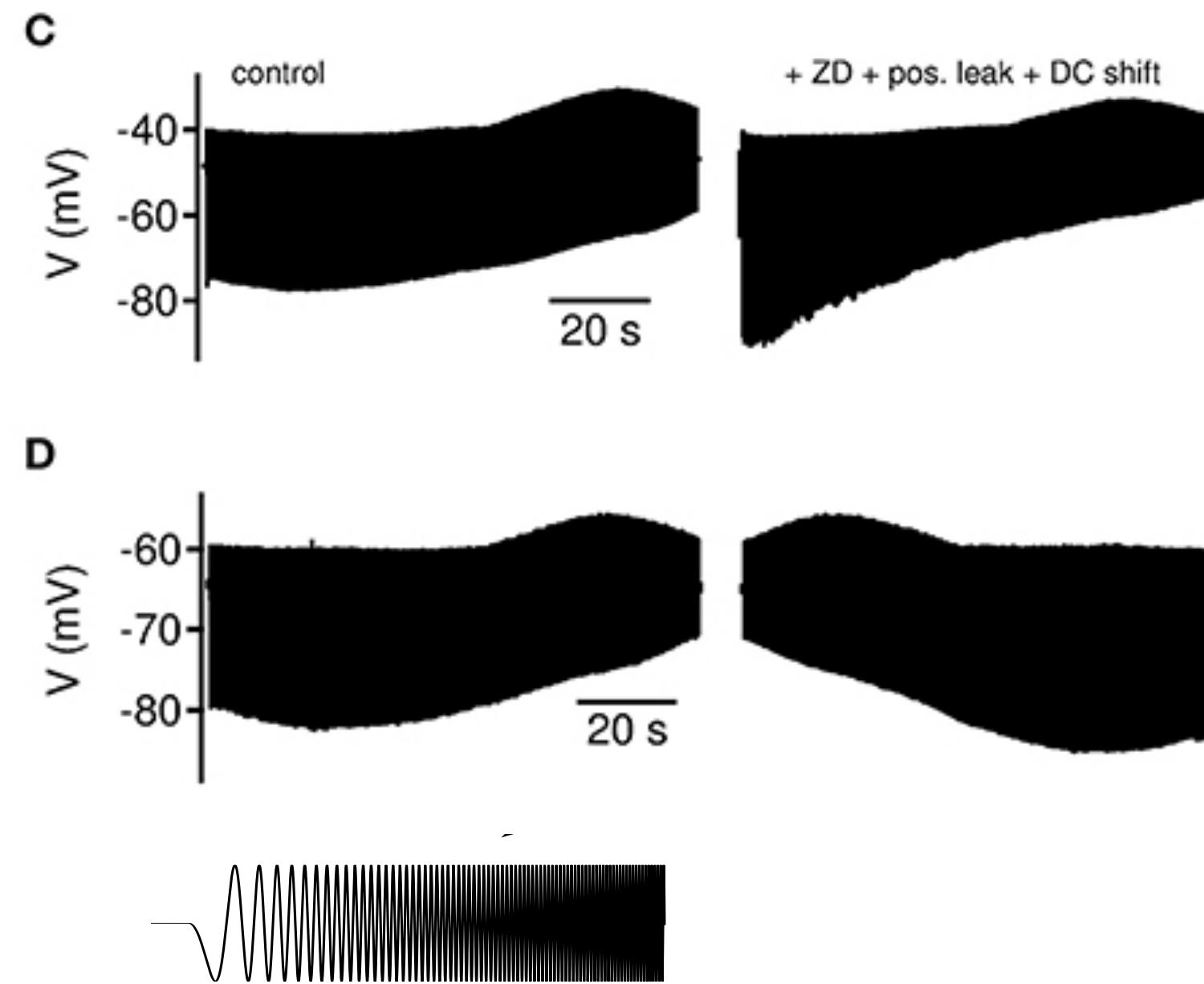
# Outline

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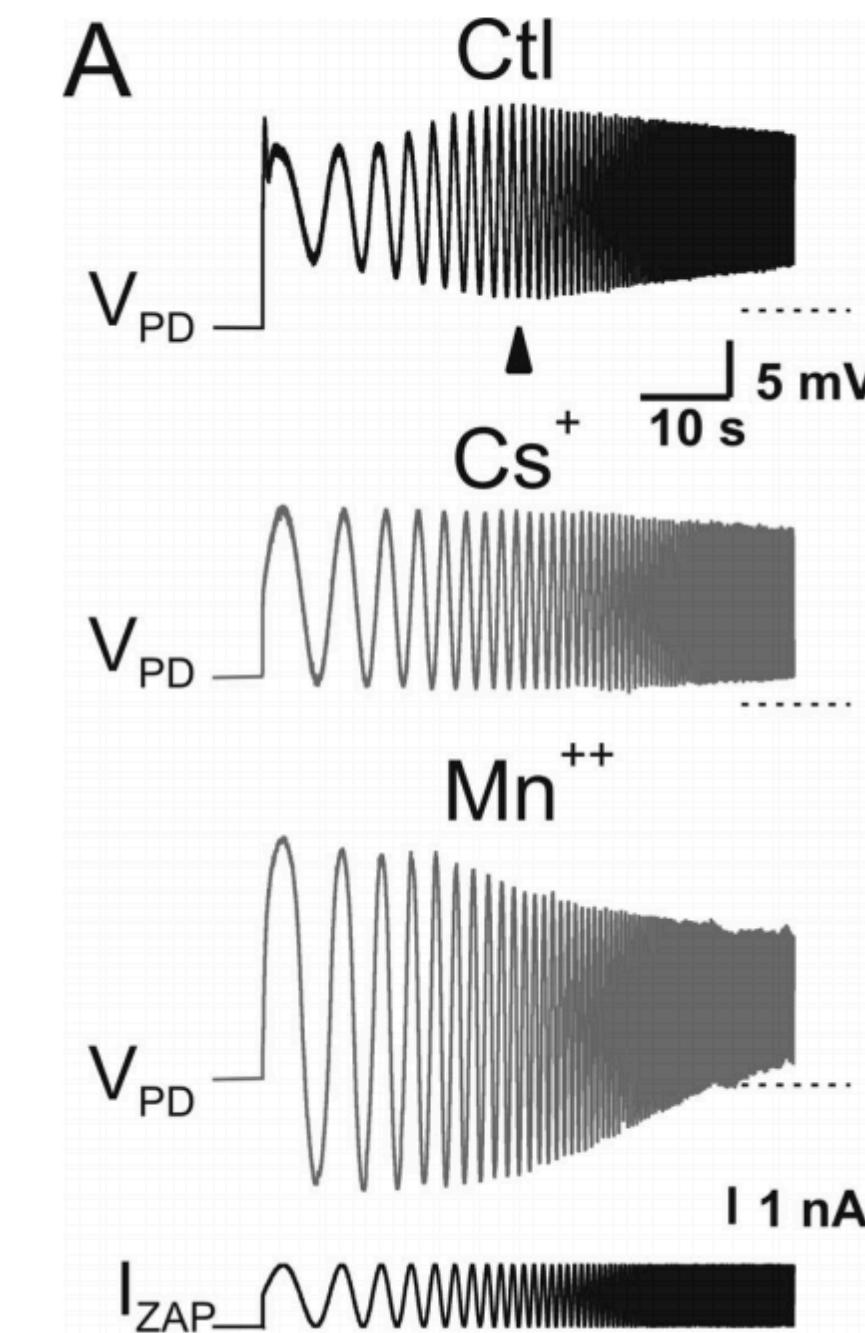
- Resonance for **suprathreshold** (spiking) behavior vs. **subthreshold regime (upper envelope)**;
- Resonance for **suprathreshold** (spiking) behavior vs. subthreshold regime (**bottom envelope**);
- **Subthreshold** resonance when a neuron is **driven by spikes**.

# Experimental observations (asymmetries)

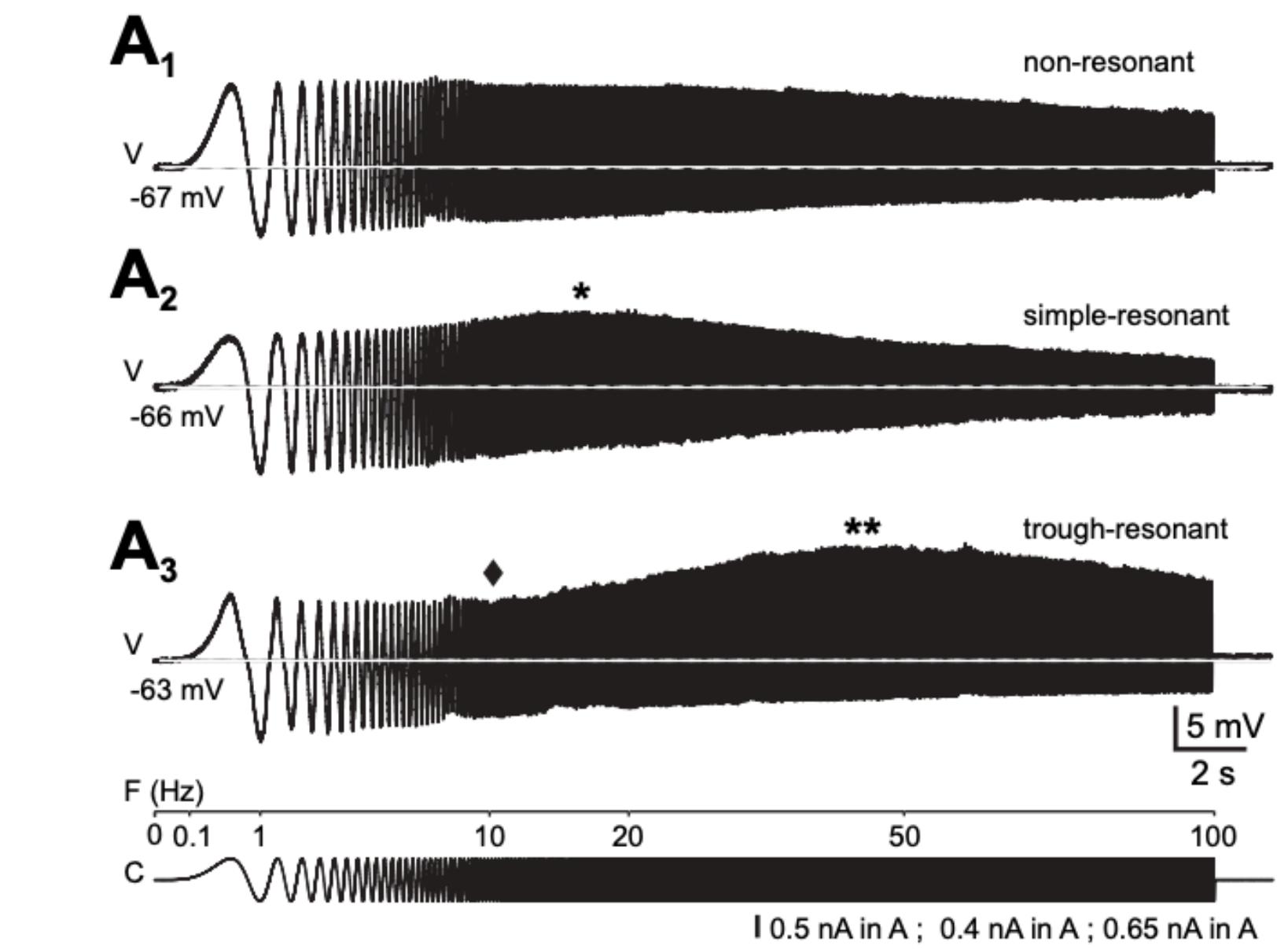
auditory brainstem neurons (mice)



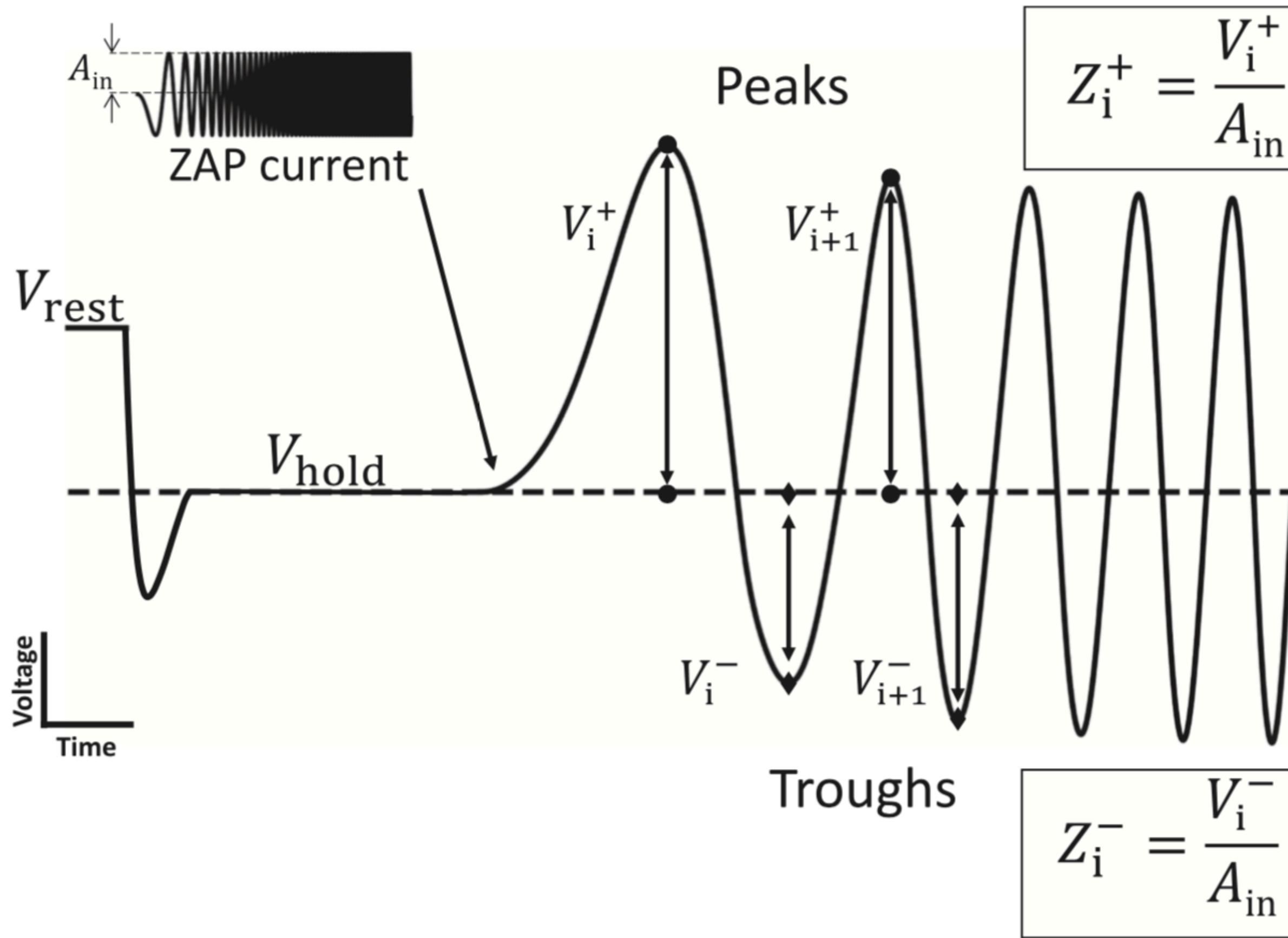
crab pyloric CPG



Frog Vestibular Neuron



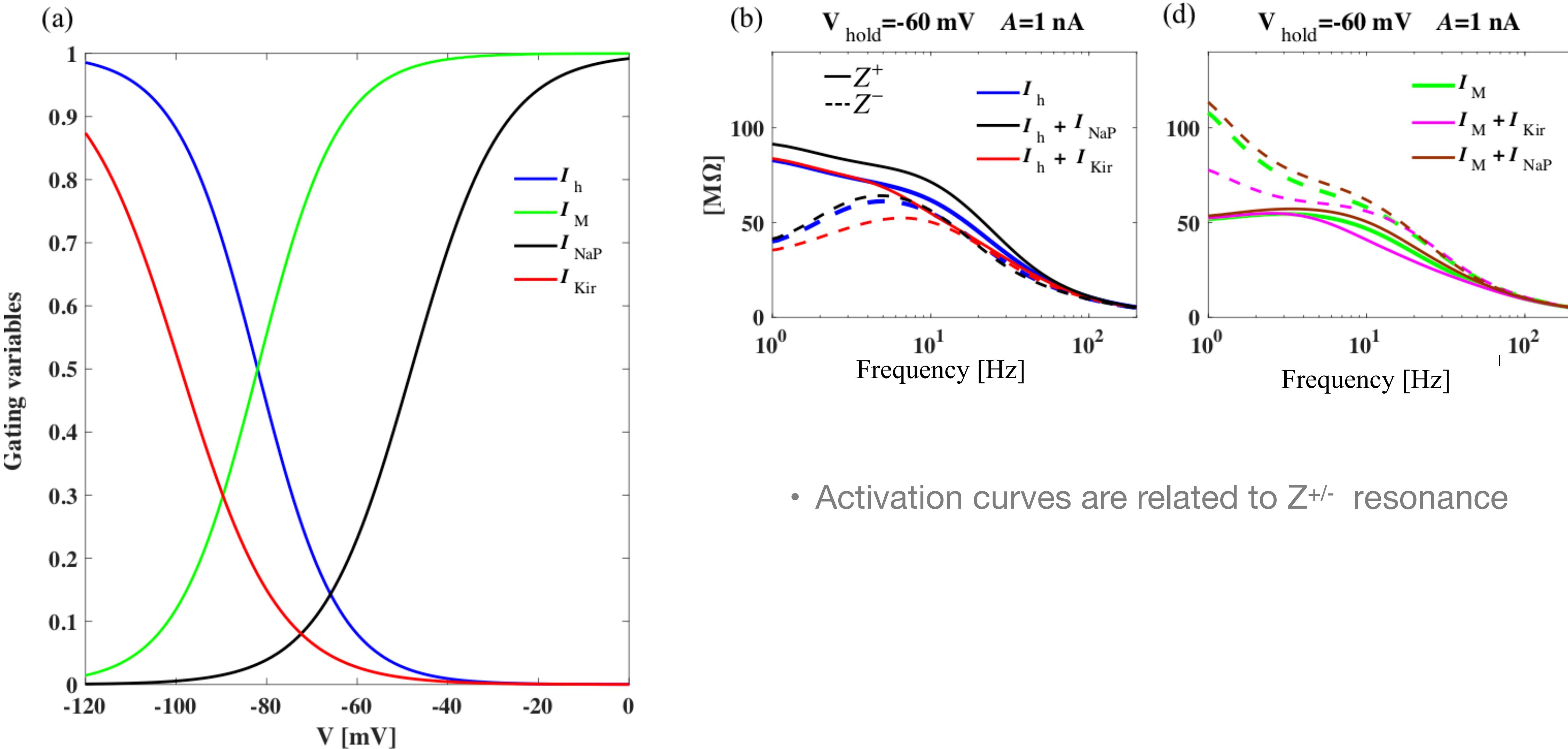
# Measuring asymmetries



Pena et al., *Chaos* **29**, 103135 (2019)

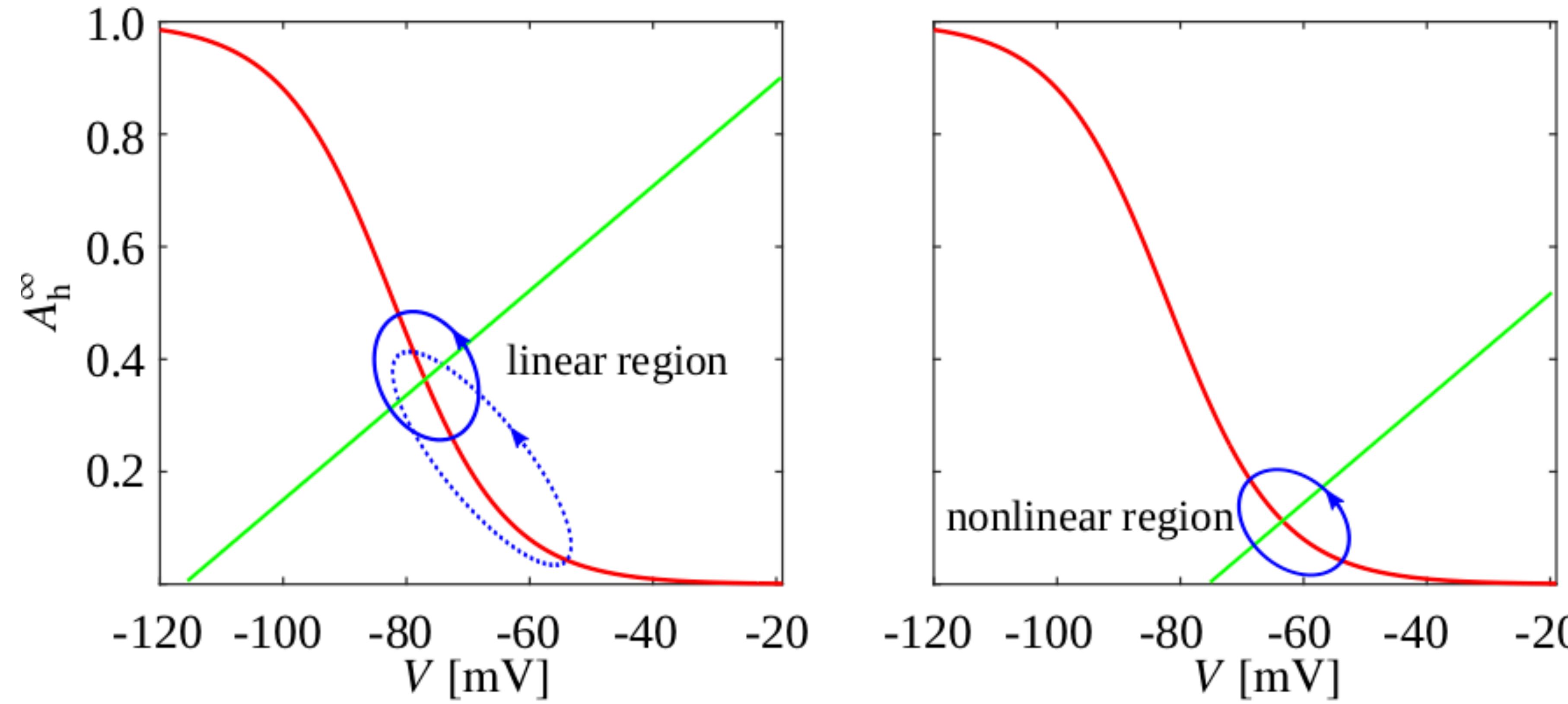
# Why asymmetries emerge?

## Biophysical explanation



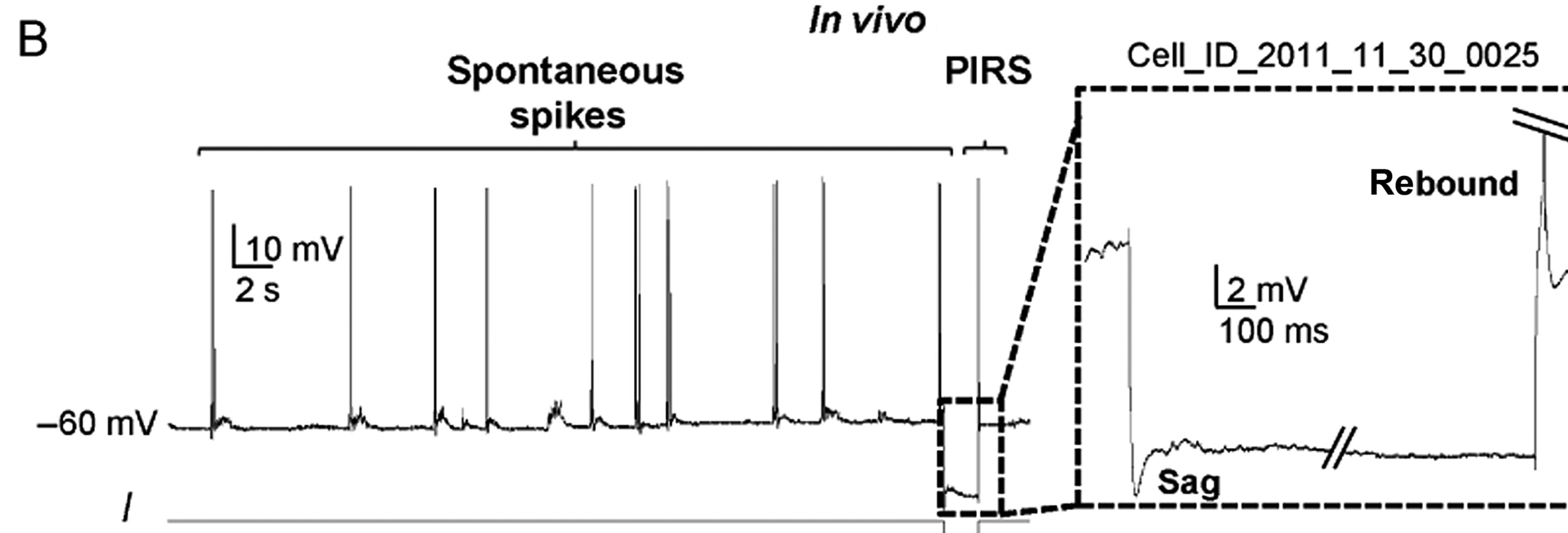
# Why asymmetries emerge?

## Dynamical explanation



Pena et al., *Chaos* **29**, 103135 (2019)

## Post-inhibitory rebound spikes in medial entorhinal cortex Layer-II stellate cells



Ferrante et al., *Cereb. Cortex* 27 (2017): 2111-2125.

# Outline

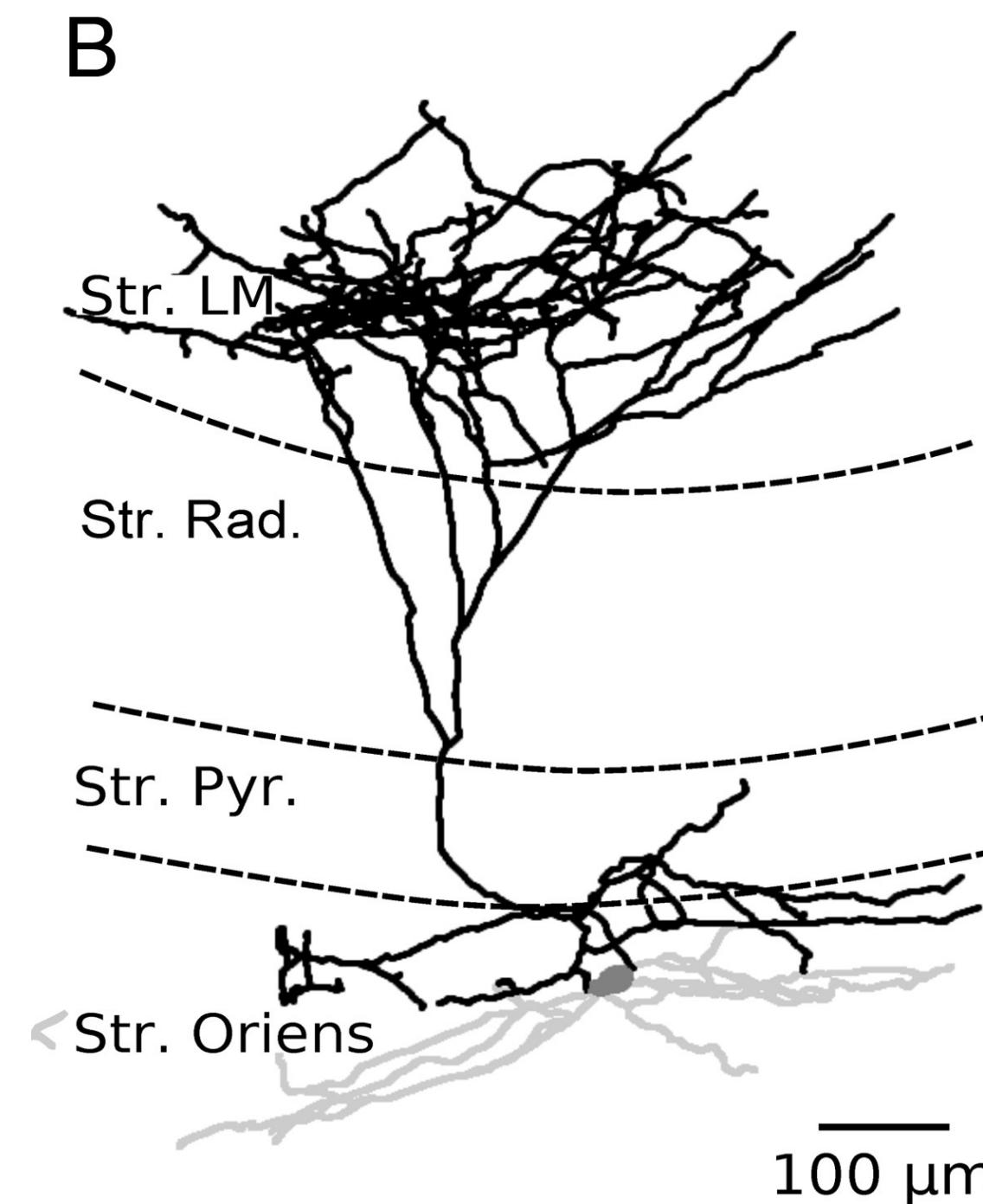
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- Resonance for **suprathreshold** (spiking) behavior vs. **subthreshold regime (upper envelope)**;
- Resonance for **suprathreshold** (spiking) behavior vs. subthreshold regime (**bottom envelope**);
- **Subthreshold** resonance when a neuron is **driven by spikes**.

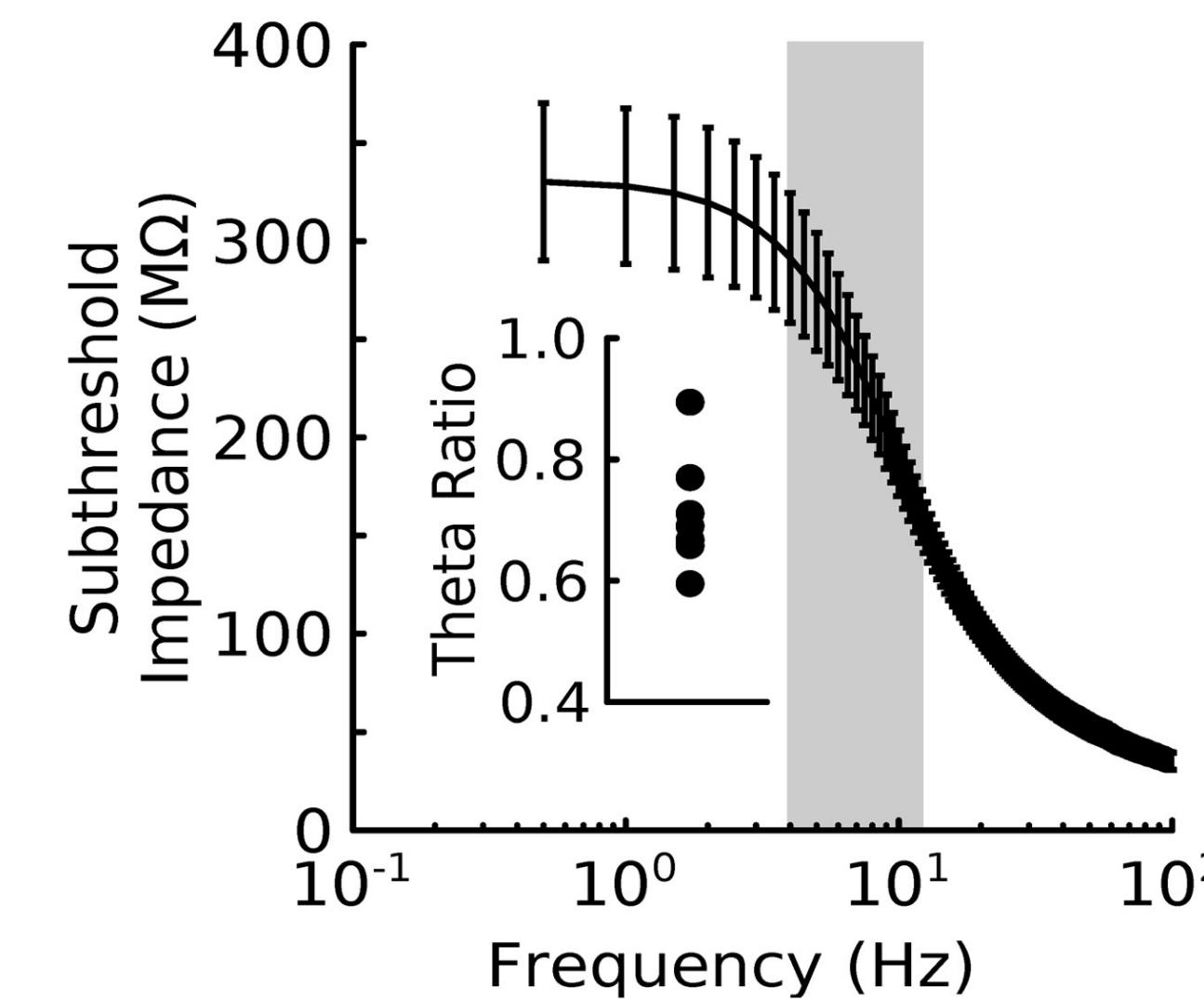
# Experimental observations (O-LM cell in hippocampus)

Kispersky et al. (2012)

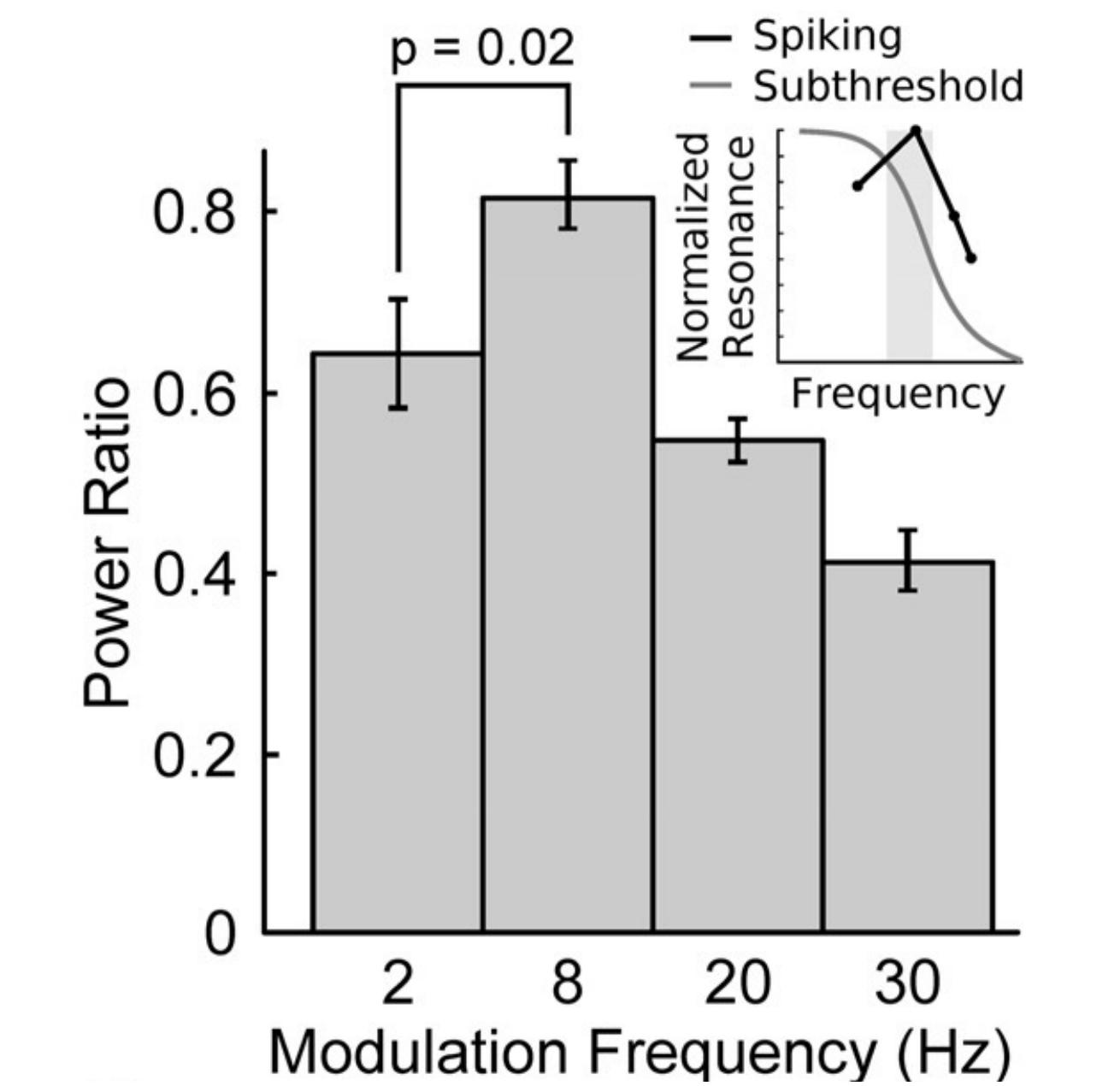
*J Neurosci* 32:3637-3651



Subthreshold impedance  
 $Z(f)$  (under white Gaussian noise)



Low-pass behavior



Spiking resonance

What does literature say about how to test resonance patterns?

## Information filtering in resonant neurons

Sven Blankenburg<sup>1,2,3</sup> · Wei Wu<sup>4</sup> · Benjamin Lindner<sup>1,3</sup> · Susanne Schreiber<sup>1,2</sup>

"Unlike resistance, impedance is a frequency-dependent relationship between the amplitudes (and phases) of **oscillatory signals**."

Hutcheon & Yarom (2000)

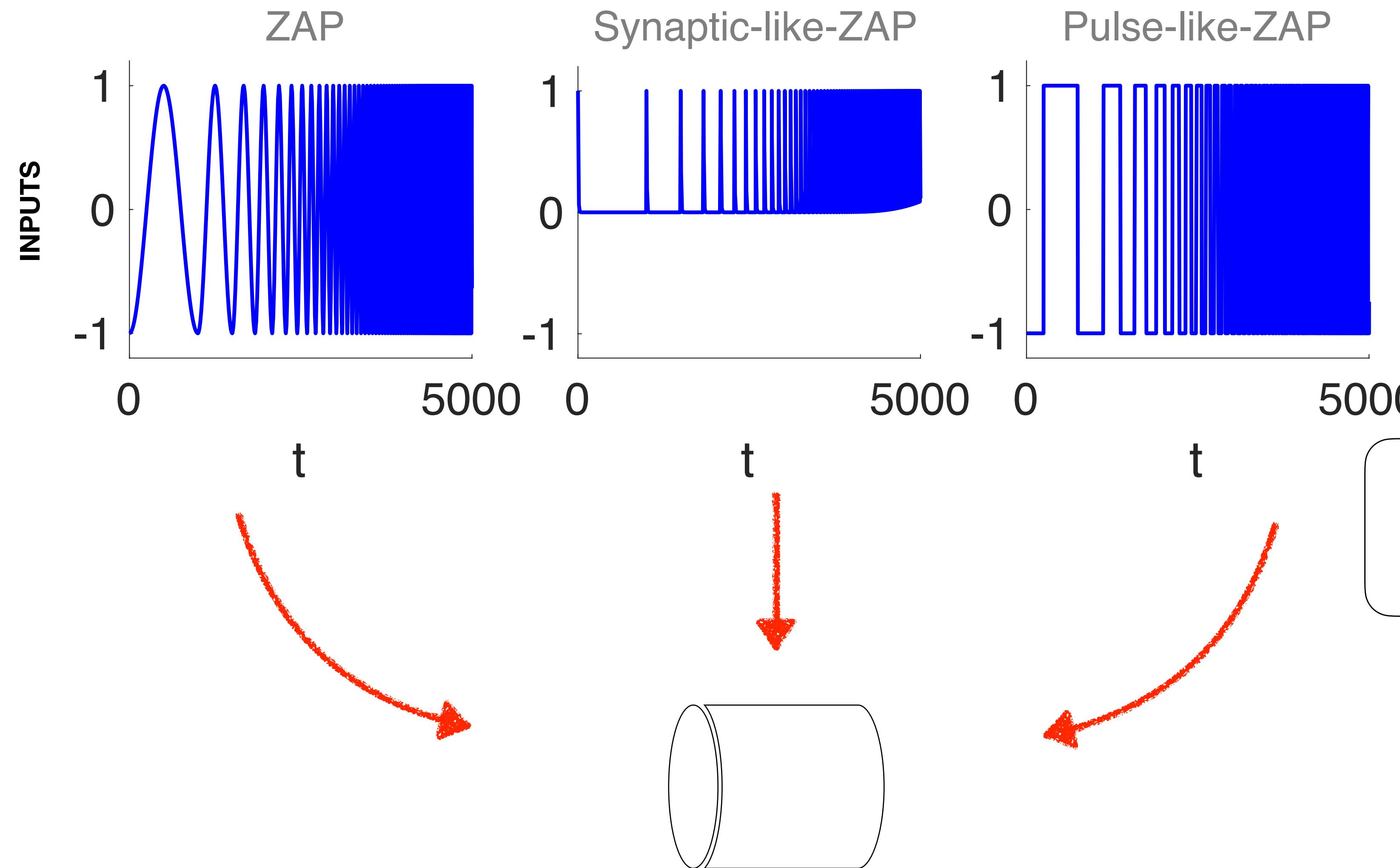
*Trends Neurosci.* 23:216-22

Impedance as a property of oscillatory signals?

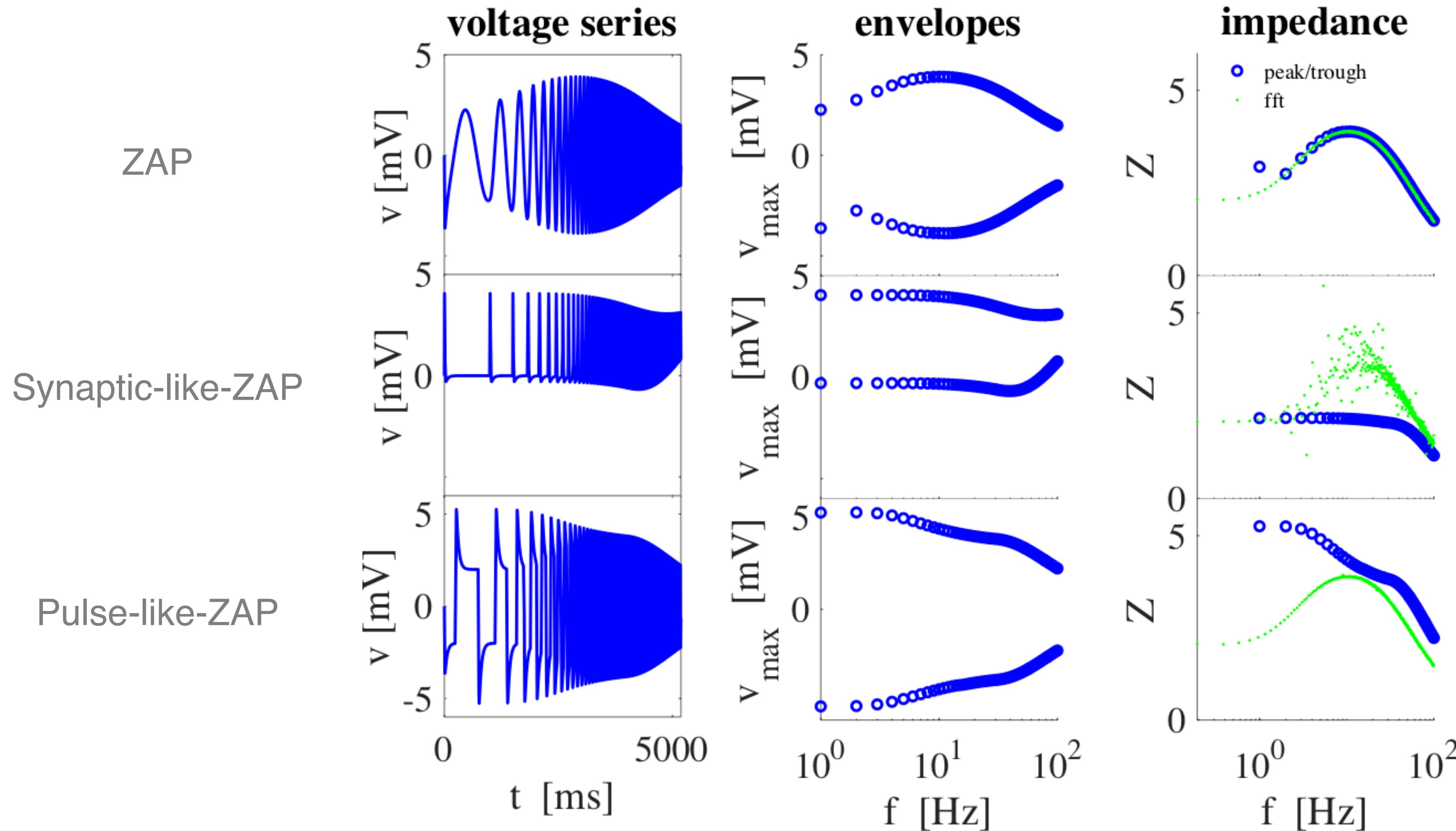
To test for resonances, stimulation can be based on any time-dependent stimuli that exhibit power in the frequency range of interest. In experiments, it is common practice to use pure sine waves or sine waves whose frequency is modulated in time (such as ZAP stimuli, see, for example Gimbarzevsky et al. 1984). Alternatively, time-dependent noise stimuli can be used as well (yielding mathematically equivalent results in linear systems). We here adopt the latter approach and model the external current signal  $s(t)$  as an Ornstein-Uhlenbeck (OU) process

$$\tau_{\text{OU}} \frac{d}{dt} s(t) = -s(t) + \xi_{\text{OU}}(t),$$

# Simple experiment with a linear neuron model

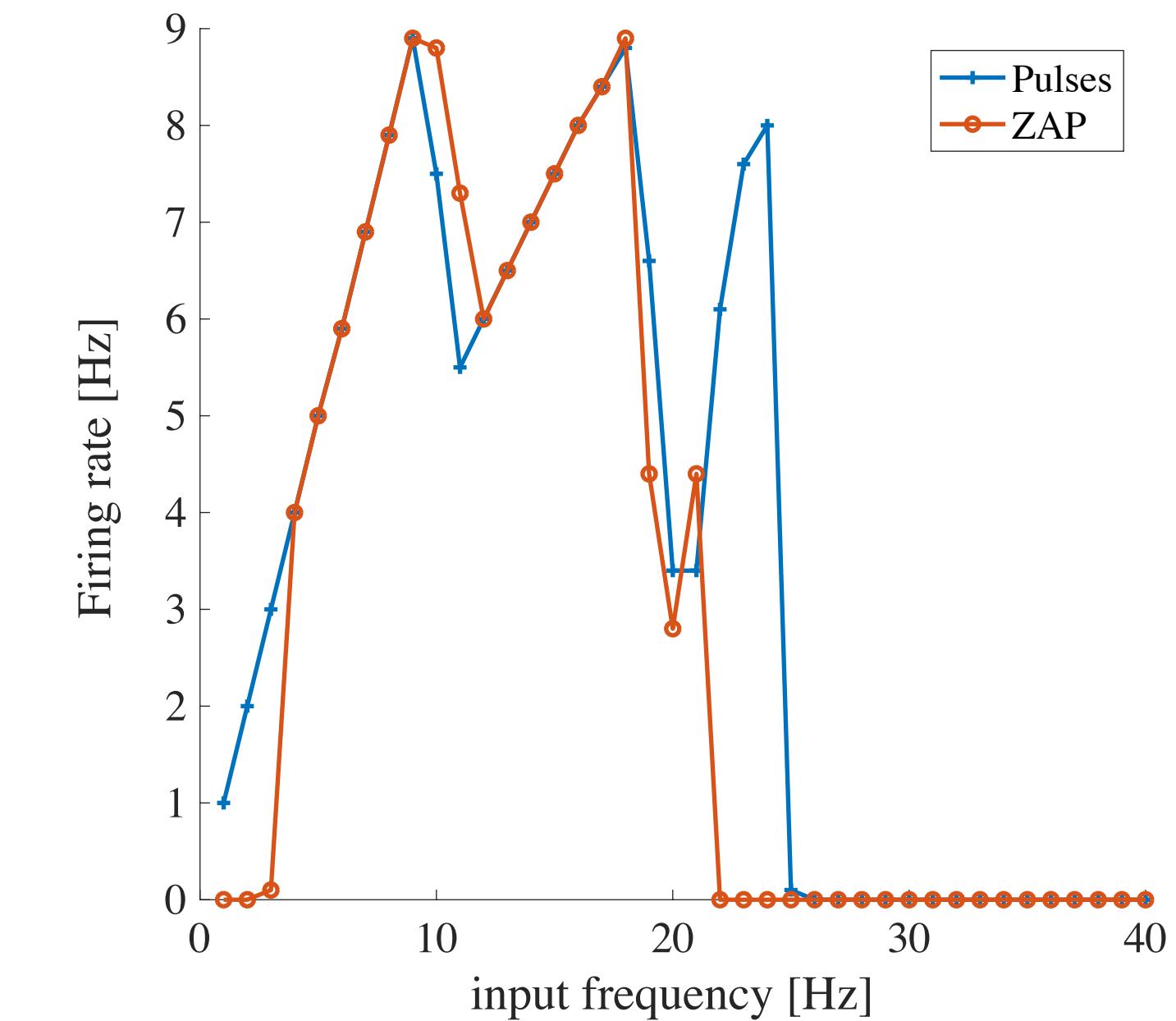
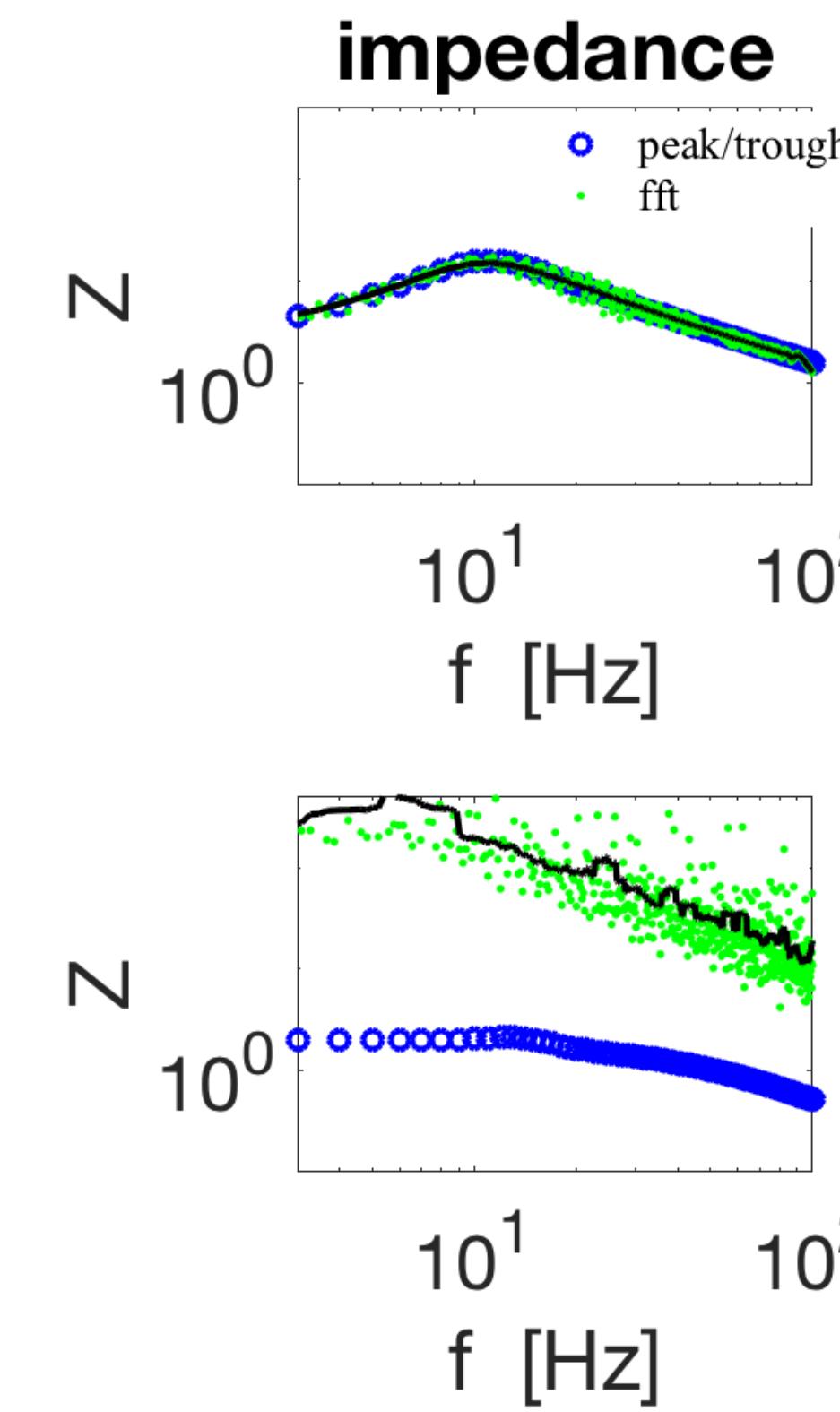
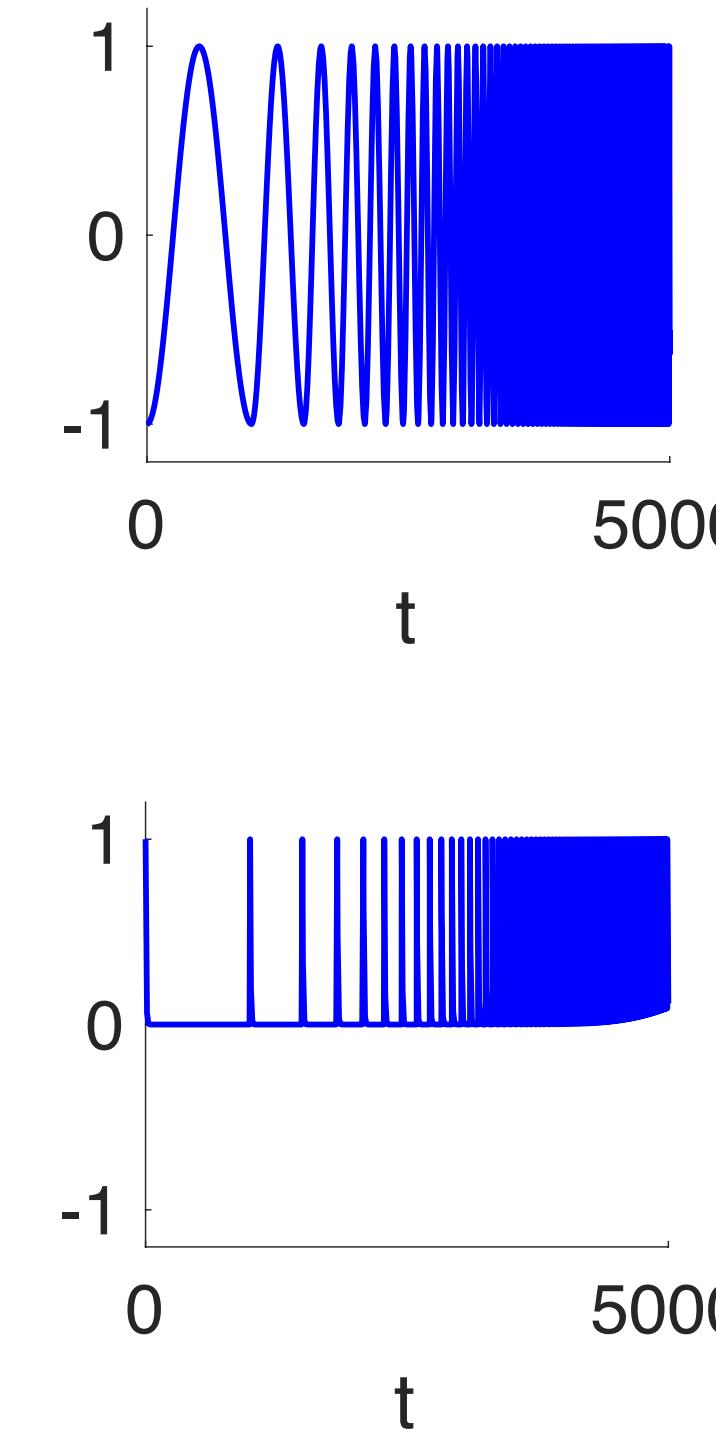
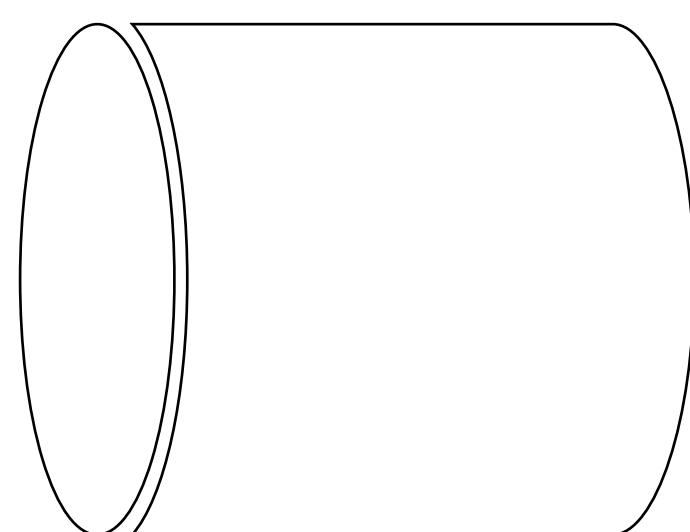


# Simple experiment with a linear neuron model



# What about spiking resonance?

Which one matters for spiking?



# Suggested literature

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## Subthreshold resonance

- Hutcheon & Yarom, *Trends Neurosci* (2000) 23:216-22

## Spiking resonance

- Rotstein, *J Comput Neurosci* (2017) 43:243–271
- Richardson et al., *J Neurophysiol* (2003) 89:2538–2554

## Asymmetries

- Pena et al., *Chaos* 29, 103135 (2019)



**Thank you very much!**