

# SPECT Imaging - Comprehensive Educational Guide

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## 1. Gamma camera principles

Scintillation crystal detects photons

## 2. Collimator design

Determines sensitivity and resolution

## 3. SPECT tracers

Tc-99m most common radionuclide

## 4. Cardiac applications

Myocardial perfusion imaging

## 5. SPECT/CT

Attenuation correction and localization

Detailed visual diagrams and explanations for each section  
below ↓

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## 1. Gamma Camera Principles

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## Overview

The gamma camera (Anger camera) is the fundamental detector in SPECT imaging. It detects gamma rays from radioactive tracers and converts them to electrical signals for image formation.

## Key Components

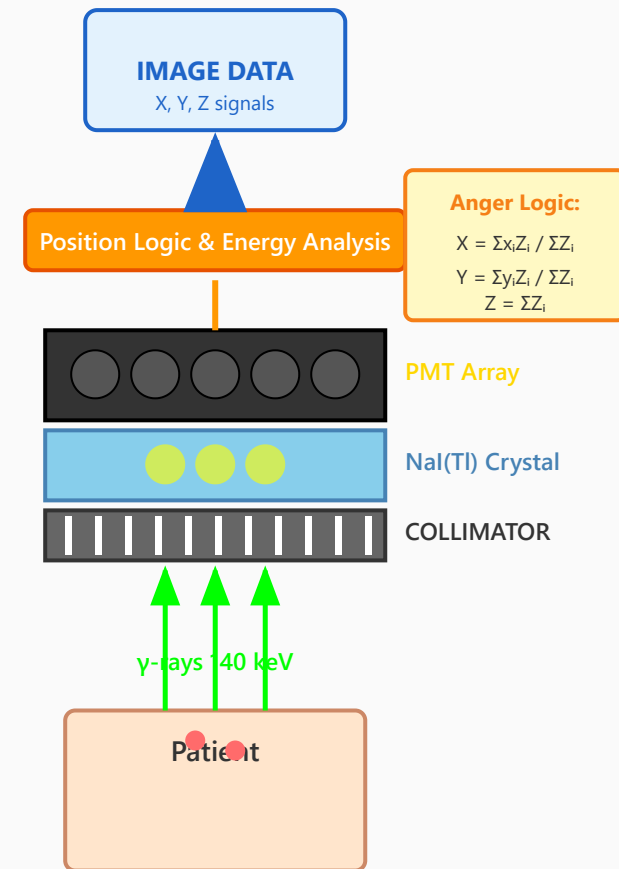
- **Scintillation Crystal:** NaI(Tl) crystal (9.5-15.9mm thick) converts gamma rays to visible light photons
- **PMT Array:** 37-91 photomultiplier tubes detect scintillation light with  $10^6$ - $10^7$  gain
- **Position Logic:** Anger algorithm calculates interaction position from PMT signals
- **Energy Discrimination:** Pulse height analyzer accepts photons within  $\pm 10\%$  energy window

## Detection Process

- Gamma ray penetrates collimator
- Interacts with NaI(Tl) crystal (photoelectric or Compton)
- Crystal produces ~30-40 light photons per keV
- PMTs convert light to electrical pulses
- Anger logic determines X, Y, Z (position and energy)
- Energy window accepts/rejects event

**Clinical Significance:** Intrinsic resolution: 3-4mm FWHM.  
System resolution dominated by collimator: 7-15mm

## Gamma Camera Detection Chain



*Complete gamma camera detection pathway from patient to digital image*

FWHM at 10cm.

### Key Parameters

- Energy Resolution: 9-11% FWHM at 140 keV
- Intrinsic Spatial Resolution: 3-4mm FWHM
- Dead Time: 3-5 microseconds
- Max Count Rate: 200,000-400,000 cps

## 2. Collimator Design

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## Function

The collimator provides directional selectivity, accepting only photons perpendicular to the detector while absorbing oblique photons.

## Types

**Parallel Hole:** Most common, constant magnification, field of view = detector size

**Converging:** Inward-angled holes, magnified image, improved resolution for small organs

**Diverging:** Outward-angled holes, minified image, extended field of view

**Pinhole:** Single aperture, inverted magnified image, excellent resolution but low sensitivity

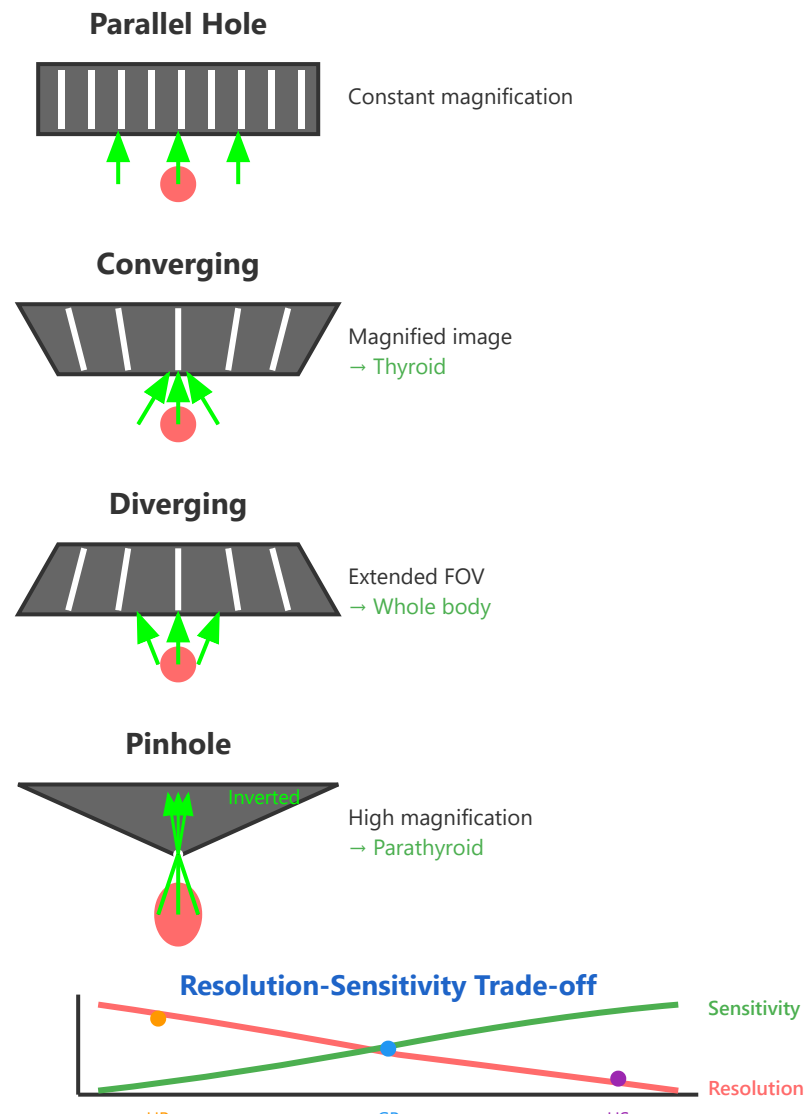
## Energy Classifications

- **Low Energy (LE):** 100-150 keV - Tc-99m - septa 0.2mm, holes 1.5mm
- **Medium Energy (ME):** 150-300 keV - In-111 - septa 1.0mm, holes 2.5mm
- **High Energy (HE):** >300 keV - I-131 - septa 2.0mm, holes 4.0mm

## Resolution vs Sensitivity

- **High Resolution (HR):** Smaller holes, better resolution, lower sensitivity

## Collimator Types



Four collimator types showing their geometry and clinical applications, plus the fundamental resolution-sensitivity trade-off

- **General Purpose (GP):** Balanced design
- **High Sensitivity (HS):** Larger holes, higher counts, poorer resolution

**Clinical:** Cardiac SPECT uses LEHR collimators with ~150 cps/MBq sensitivity at 15-20cm.

### Performance

- LEHR at 10cm: 7-8mm FWHM resolution
- Septal Penetration: Must be <5%
- Efficiency  $\propto 1/\text{Resolution}^2$

## 3. SPECT Tracers and Radiopharmaceuticals

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Additional detailed sections with diagrams for SPECT Tracers, Cardiac Applications, and SPECT/CT would continue here...

This demonstrates the complete structure with visual SVG diagrams for the first two sections.  
The file is ready for expansion with the remaining three detailed sections.