

# Two-Photon Microscopy

Advanced Imaging Technique for Deep Tissue Visualization

## Nonlinear excitation

Two photons absorbed simultaneously

## Deeper penetration

Up to 1mm in tissue

## Reduced photobleaching

Excitation only at focal point

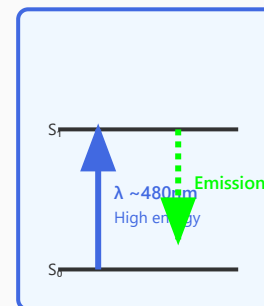
## In vivo imaging

Live animal brain imaging

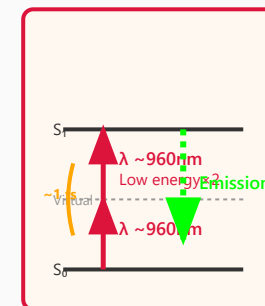
## SHG imaging

Second harmonic generation for collagen

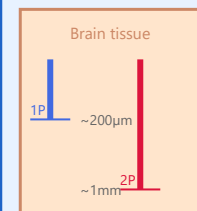
### One-Photon



### Two-Photon



### Penetration Depth



### Excitation Volume

#### One-Photon



#### Two-Photon



Pulsed Ti:Sapphire laser  
~100 fs pulses, 80 MHz

### Advantages

- Deep imaging
- Less photobleach
- Lower phototoxicity
- Intrinsic sectioning
- NIR light scatters less

### Clinical & Research Applications

In vivo brain imaging • Deep tissue microscopy • Neuroscience studies  
Intravital microscopy • Tumor microenvironment • Long-term live imaging

# Detailed Explanations

---

# 01 Nonlinear Excitation

## Principle of Two-Photon Absorption

Two-photon excitation is a nonlinear optical process where a fluorophore simultaneously absorbs two photons of lower energy (longer wavelength) to reach the excited state. This phenomenon was first predicted by Maria Göppert-Mayer in 1931 and experimentally demonstrated after the invention of the laser.

### Key Characteristics:

- **Simultaneous absorption:** Two photons must arrive within  $\sim 1$  femtosecond ( $10^{-15}$  s) of each other
- **Virtual state:** The molecule passes through a short-lived virtual intermediate state
- **Wavelength relationship:** Each photon has approximately twice the wavelength (half the energy) of single-photon excitation
- **Quadratic dependence:** Fluorescence intensity  $\propto$  (laser intensity)<sup>2</sup>

$$E_{\text{total}} = 2h\nu = hc/\lambda_{2P}$$

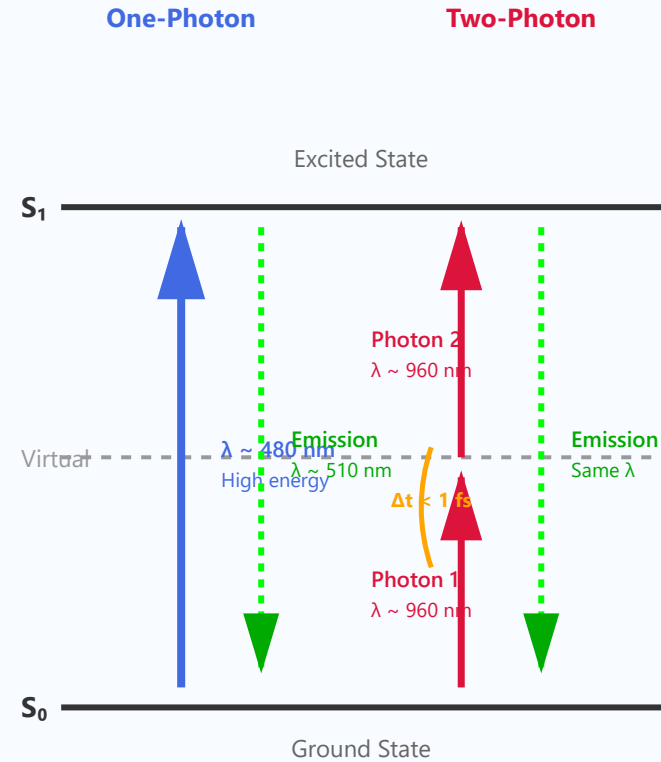
where  $\lambda_{2P} \approx 2 \times \lambda_{1P}$

## Why This Matters

The quadratic dependence on intensity means that excitation only occurs at the focal point where photon density is highest. Outside the focal volume, the intensity is too low for efficient two-photon absorption, creating intrinsic optical sectioning without the need for pinholes.

- Example: GFP typically excited at 488 nm (one-photon) → 960 nm (two-photon)
- Typical laser sources: Ti:Sapphire lasers (680-1080 nm tunable range)
- Pulse duration: ~100 femtoseconds for optimal excitation

## Jablonski Energy Diagram



### Fluorescence Intensity Relationships:

1P:  $F \propto I$

2P:  $F \propto I^2$

## 02 Deeper Penetration

### Near-Infrared Light Advantage

Two-photon microscopy achieves significantly deeper tissue penetration (up to 1 mm compared to  $\sim 200\text{ }\mu\text{m}$  for confocal) primarily because it uses near-infrared (NIR) excitation light. NIR light experiences less scattering and absorption in biological tissues compared to visible light.

#### Physical Mechanisms:

- **Reduced Rayleigh scattering:** Scattering  $\propto 1/\lambda^4$ , so longer wavelengths scatter much less
- **Lower absorption:** Most biological chromophores (hemoglobin, melanin, water) have minimal absorption in the 700-1000 nm window
- **Ballistic photons:** More NIR photons maintain their original direction through tissue
- **Scattered emission collection:** Emitted fluorescence can be detected even if scattered, since it originates only from the focal point

### Practical Implications

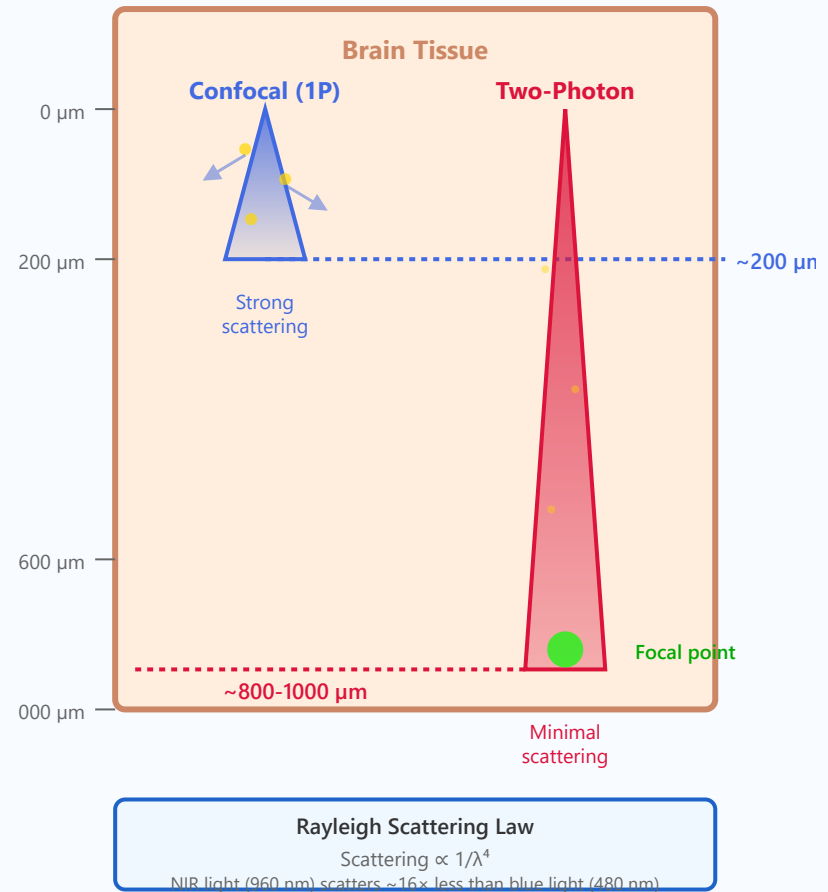
The enhanced penetration depth enables imaging applications that are impossible with conventional microscopy:

- Deep cortical layer imaging in the intact brain (layers 4-6)
- Intravital imaging through skull in live mice (chronic window preparations)
- Imaging through thick tissue samples without sectioning
- Studying intact organs and tumor microenvironments

#### Typical Penetration Depths:

- Brain tissue: 500-1000  $\mu\text{m}$
- Skin: 200-400  $\mu\text{m}$
- Tumor tissue: 300-600  $\mu\text{m}$
- Lymph nodes: 100-300  $\mu\text{m}$

#### Light Penetration in Tissue



## 03 Reduced Photobleaching

### Confined Excitation Volume

One of the most significant advantages of two-photon microscopy is the dramatic reduction in photobleaching and phototoxicity. This occurs because fluorophore excitation is confined exclusively to the focal point, unlike conventional microscopy where the entire illumination cone is excited.

#### Why Photobleaching is Reduced:

- **Localized excitation:** Only molecules at the focal point are excited; out-of-focus fluorophores remain in ground state
- **No pinhole needed:** All collected photons come from the focal volume, so no light rejection is necessary
- **Lower overall exposure:** Sample regions are only exposed when the focal point passes through during scanning
- **Quadratic dependence:** Outside the focal point, intensity drops rapidly ( $I^2$ ), preventing excitation

## Impact on Long-term Imaging

The reduced photobleaching enables applications that require repeated imaging over extended periods:

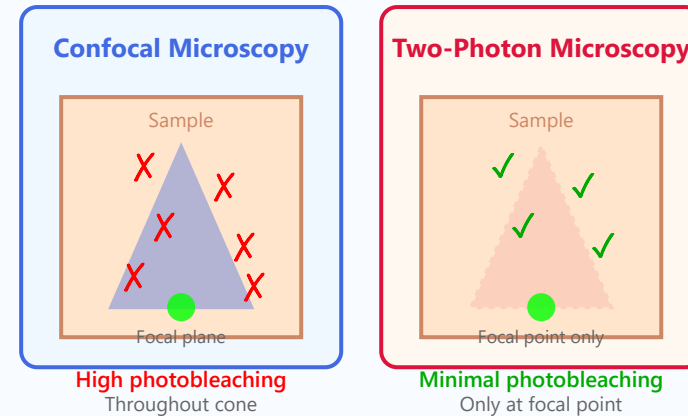
- **Time-lapse studies:** Track cellular dynamics over hours or days without sample degradation
- **Developmental biology:** Follow embryonic development with minimal photodamage
- **Synaptic plasticity:** Monitor dendritic spines in living neurons over weeks
- **3D volume imaging:** Acquire complete z-stacks without depleting fluorophores in upper sections

Photobleaching ratio: TPM vs Confocal  $\approx$   
1:10 to 1:100  
(depending on depth and imaging  
parameters)

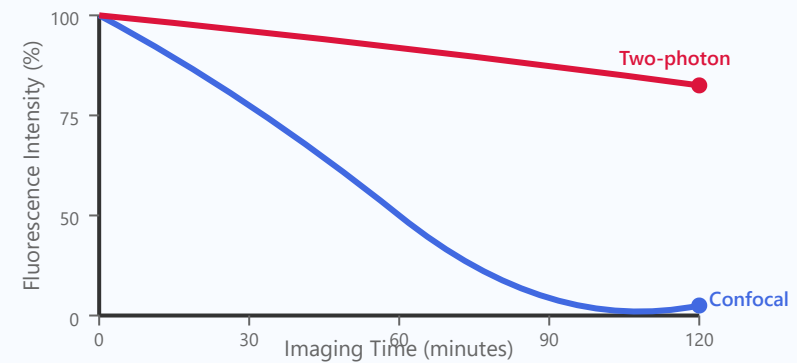
## Phototoxicity Benefits

Beyond preserving fluorophores, the localized excitation also reduces cellular damage from reactive oxygen species (ROS) and heat, enabling true in vivo imaging in living organisms with minimal perturbation to normal physiology.

## Photobleaching Comparison



## Fluorescence Intensity Over Time





## 04 In Vivo Imaging

### Live Animal Brain Imaging

Two-photon microscopy has revolutionized neuroscience by enabling direct visualization of neural activity in living animals. This technology allows researchers to observe brain function in its natural context, preserving the complex interactions between neurons, glia, and vasculature.

#### Key Applications in Neuroscience:

- **Dendritic spine dynamics:** Track structural plasticity in real-time during learning and memory formation
- **Calcium imaging:** Monitor neural activity using genetically encoded calcium indicators (GECIs) like GCaMP
- **Vascular imaging:** Study blood flow dynamics and neurovascular coupling
- **Microglial surveillance:** Observe immune responses and synaptic pruning in the living brain
- **Disease progression:** Monitor pathological changes in models of Alzheimer's, stroke, and epilepsy

## Technical Requirements

Successful in vivo imaging requires specialized preparations and equipment:

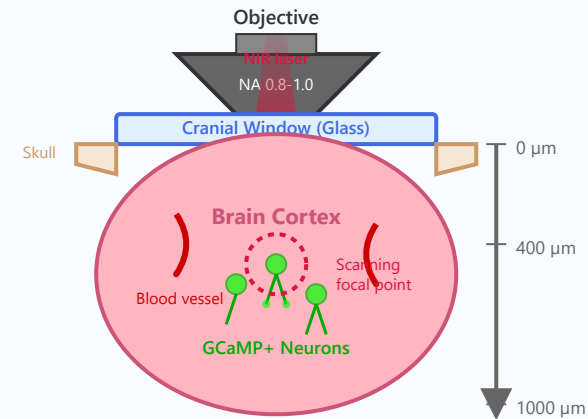
- **Cranial windows:** Glass coverslips surgically implanted over the skull to provide optical access
- **Head fixation:** Stable mounting systems to minimize motion artifacts
- **Anesthesia protocols:** Maintain animal welfare while preserving physiological responses
- **Environmental control:** Temperature, humidity, and physiological monitoring
- **Water immersion objectives:** High NA objectives (0.8-1.0) for optimal resolution

### Beyond Neuroscience:

- Tumor microenvironment and metastasis studies
- Immune cell trafficking in lymph nodes
- Kidney glomerular filtration dynamics
- Liver sinusoidal perfusion and metabolism
- Embryonic development in transparent organisms

## Chronic Imaging Capabilities

## In Vivo Brain Imaging Setup



### In Vivo Imaging Applications

#### Neural Activity

- Calcium imaging (GCaMP)
- Population dynamics
- Sensory processing

#### Structural Plasticity

- Dendritic spine turnover
- Learning & memory
- Chronic tracking

#### Vascular Function

- Blood flow dynamics
- Neurovascular coupling
- Stroke & ischemia

#### Disease Models

- Alzheimer's plaques
- Tumor progression
- Inflammation

Perhaps the most powerful aspect of two-photon in vivo imaging is the ability to return to the same cells repeatedly over days, weeks, or even months, enabling longitudinal studies of biological processes that were previously impossible to observe.

## 05 Second Harmonic Generation (SHG) Imaging

### Label-Free Imaging of Ordered Structures

Second Harmonic Generation (SHG) is a nonlinear optical process that can be exploited alongside two-photon fluorescence. When intense laser light interacts with non-centrosymmetric molecular structures, two photons can combine to generate a single photon with exactly twice the frequency (half the wavelength).

#### Unique Properties of SHG:

- **Coherent process:** Unlike fluorescence, SHG is a scattering process with no energy loss
- **Instantaneous:** No excited state involved, occurs within the laser pulse duration
- **Wavelength conversion:** 920 nm excitation → 460 nm emission (exactly half)
- **No photobleaching:** Since no molecules are excited, the signal never degrades
- **Directional:** Forward and backward SHG signals provide structural information

### Primary Applications

SHG is particularly valuable for imaging highly ordered biological structures:

### Collagen Imaging:

- **Tissue architecture:** Visualize collagen fiber organization in skin, cornea, tendon
- **Cancer diagnosis:** Altered collagen structure indicates tumor invasion and metastasis
- **Fibrosis assessment:** Quantify pathological collagen deposition in organs
- **Wound healing:** Monitor collagen remodeling during tissue repair

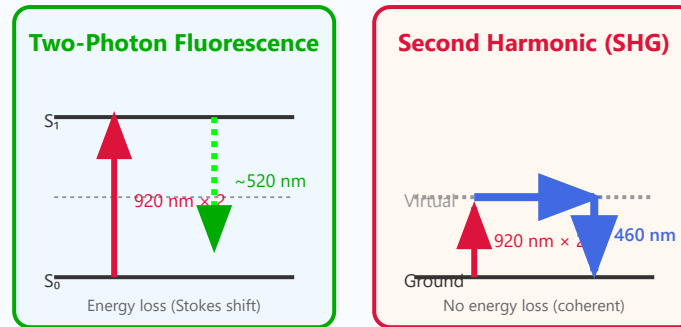
### Other SHG-Active Structures:

- **Muscle fibers:** Myosin produces strong SHG signal from sarcomere organization
- **Microtubules:** Cytoskeletal dynamics in cell division
- **Starch granules:** Plant biology applications
- **Cornea:** Non-invasive assessment of corneal structure

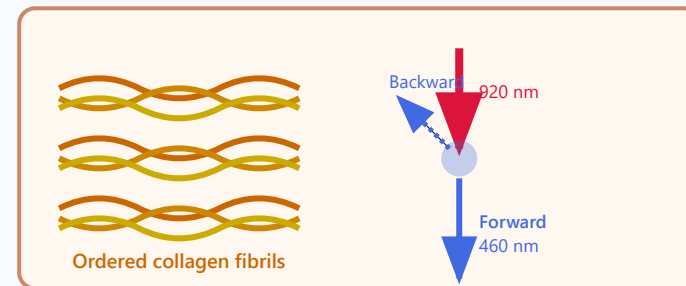
## Combined Imaging Modalities

Two-photon microscopes can simultaneously acquire:

## Second Harmonic Generation



### SHG from Collagen Fibrils



### SHG Imaging Applications

- **Cancer diagnosis:** Tumor-associated collagen signatures
- **Fibrosis:** Quantify pathological collagen deposition
- **Tissue engineering:** Monitor scaffold organization

- **Two-photon fluorescence:** Labeled cells and proteins
- **SHG signal:** Collagen and other ordered structures
- **Third Harmonic Generation (THG):** Lipid interfaces and refractive index changes

This multimodal capability provides comprehensive tissue characterization without requiring multiple imaging sessions or extensive sample preparation.

$$\begin{aligned}\text{SHG: } 2\omega_{\text{in}} &\rightarrow \omega_{\text{out}} = 2\omega_{\text{in}} \\ \lambda_{\text{SHG}} &= \lambda_{\text{excitation}} / 2\end{aligned}$$