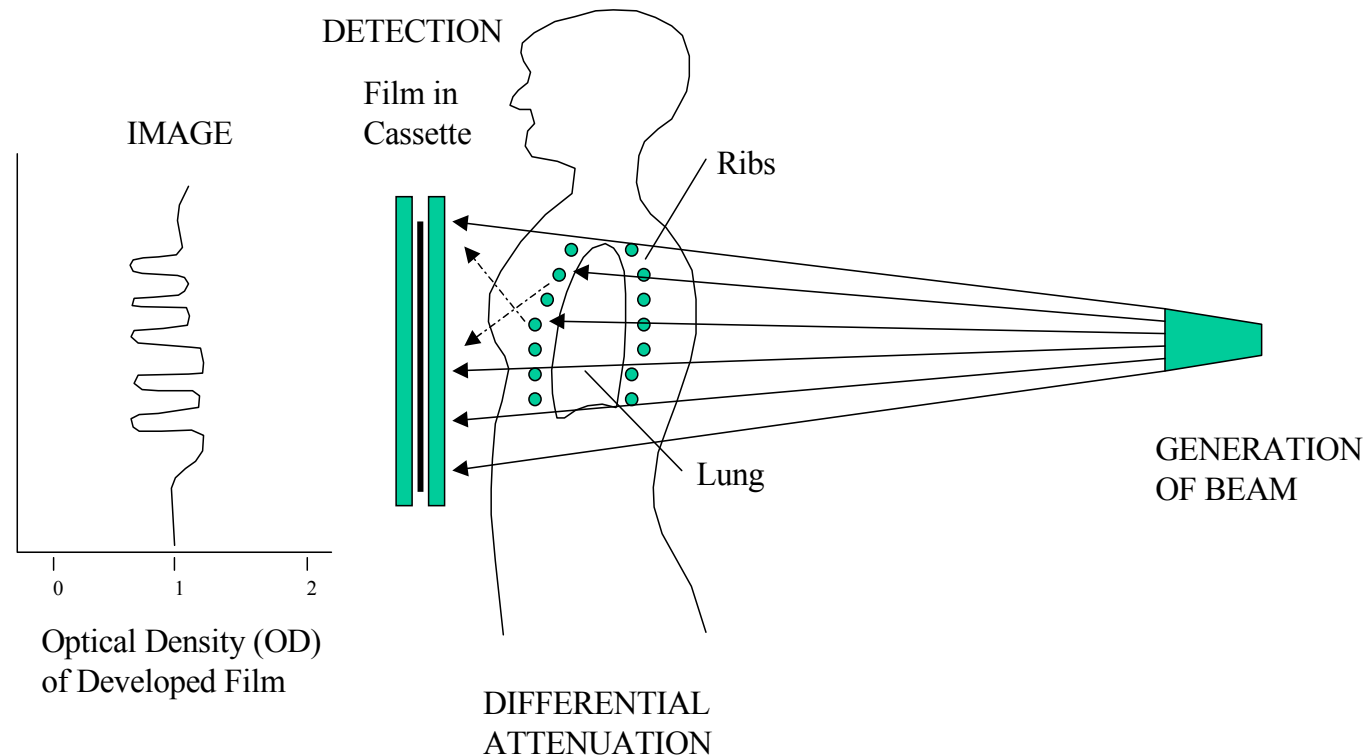


## Handout #3

### Projection Radiography

#### 3.1 Screen-film System

❖ Schematic of projection radiography



❖ In this system, film is used to record images.

## The x-ray film has several major functions:

- (a) Detector
- (b) Display device
- (c) Archival medium

More exposure, the darker the film

The film itself is very **inefficient** under direct x-ray exposure, only about **5%** of x-ray photons can be absorbed by the film and react with the emulsion. Therefore, **scintillating screens** (phosphor) are used.

### ❖ Screen-film combination

- Scintillating screen: convert high energy x-ray photons to a large number of light photons
- Film: record an image

The fraction of X-rays absorbed by a calcium tungstate screen is about **20-40%** depending on the speed (**determined mainly by screen thickness**), while rare earth screens absorb about **60%**.

- ❖ The x-ray quantum efficiency (absorption efficiency) of the scintillating screen is much higher than the film.

### Example 1:

**Assume:** a 50KeV x-ray photon is absorbed in a calcium tungstate screen that emits most of its light at a wavelength of 430 nm. The energy of the light photon is:

$$\lambda \text{ (nm)} = 1.24 / E \text{ (KeV)}$$

$$E \text{ (KeV)} = 1.24 / 430 = 0.00288 \text{ KeV} = 3 \text{ eV}$$

The energy of the light photon at a wavelength of 430 nm is about 3 eV.

Therefore the number of light photons produced is:

$$(50,000 \text{ eV} / 3 \text{ eV}) \times 0.05 = 17,000 \times 0.05 = 850$$

**The 5% efficiency** in the above calculation is termed the **Intrinsic conversion efficiency** of the phosphor, (the ratio of the light energy liberated by the crystal to the x-ray energy absorbed).

The Intrinsic conversion efficiency of rare earth screens is **about 12-18%**

Among all of these 850 photons, **about half of them (?)**, say 425, will reach the film.

## Example 2:

Assume 1000 x-ray photons irradiate both screen-film and film alone:

	Screen-film	Film alone
<b>X-ray photons absorbed by</b>	400	50
<b>Light photons produced</b>	$400 \times 850 = 340,000$	
<b>Light photons reaching film</b>	170,000	
<b>Latent image centers formed</b>	1700	50

The intensification factor =  $1700 / 50 = 34$

**The intensification factor** = (X-ray exposure required without screen) / (x-ray exposure required with screen)

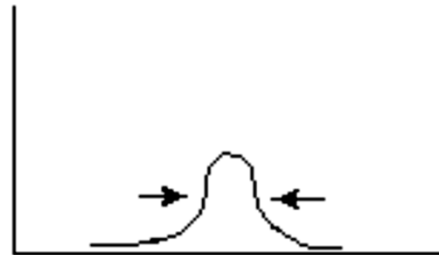
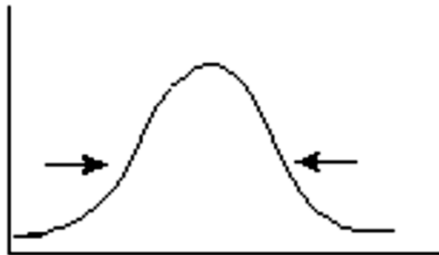
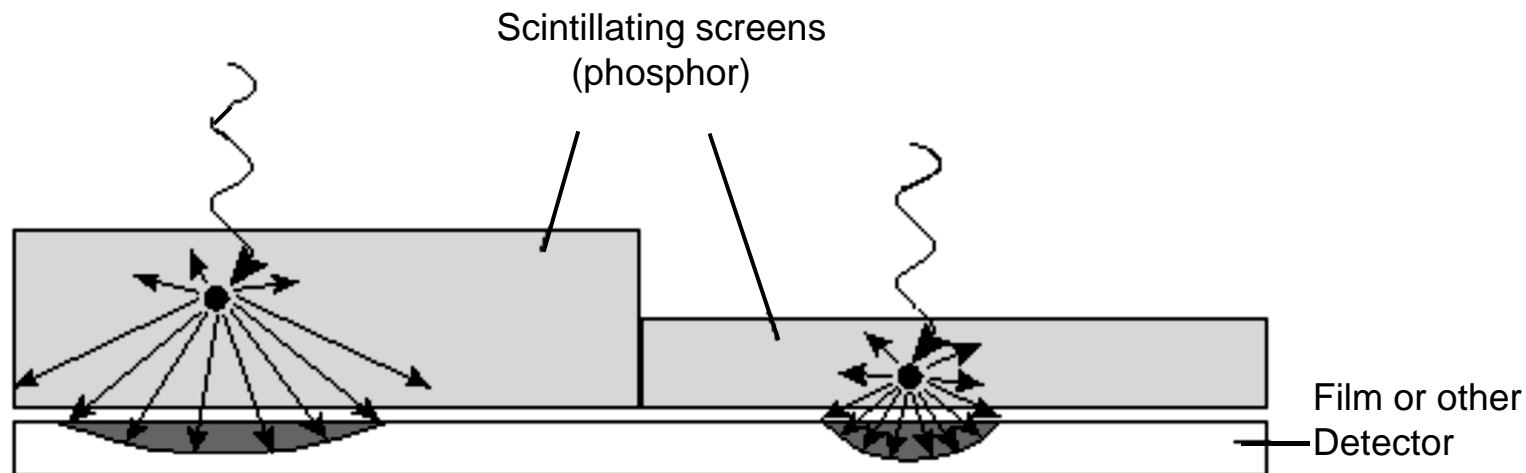
**Note:** At this point, let us simply define the latent image center as the end product of the photographic effect of light or x-rays on the film emulsion.

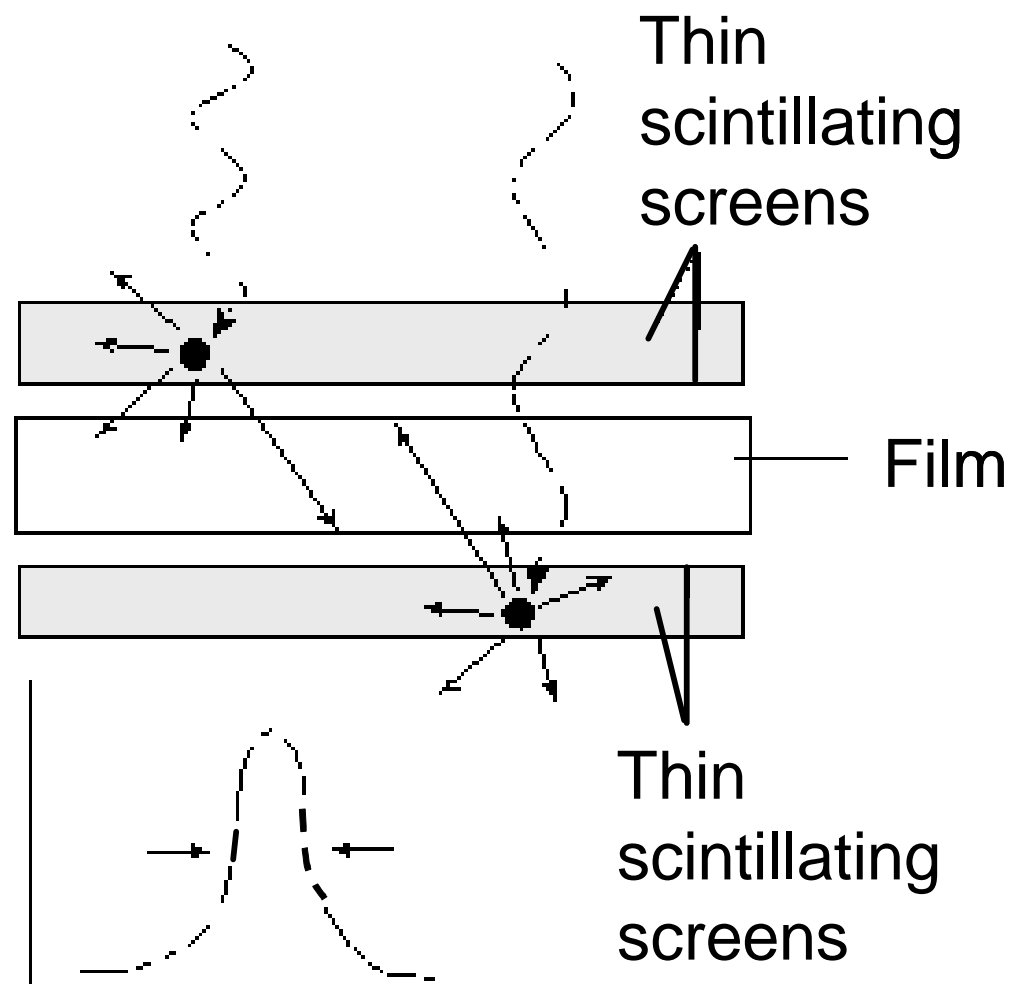
❖ The screen amplifies the photographic effect of x-rays

## ❖ Screen thickness considerations:

In order to absorb more x-ray photons: Thicker screen

In order to have higher resolving power: Thinner screen

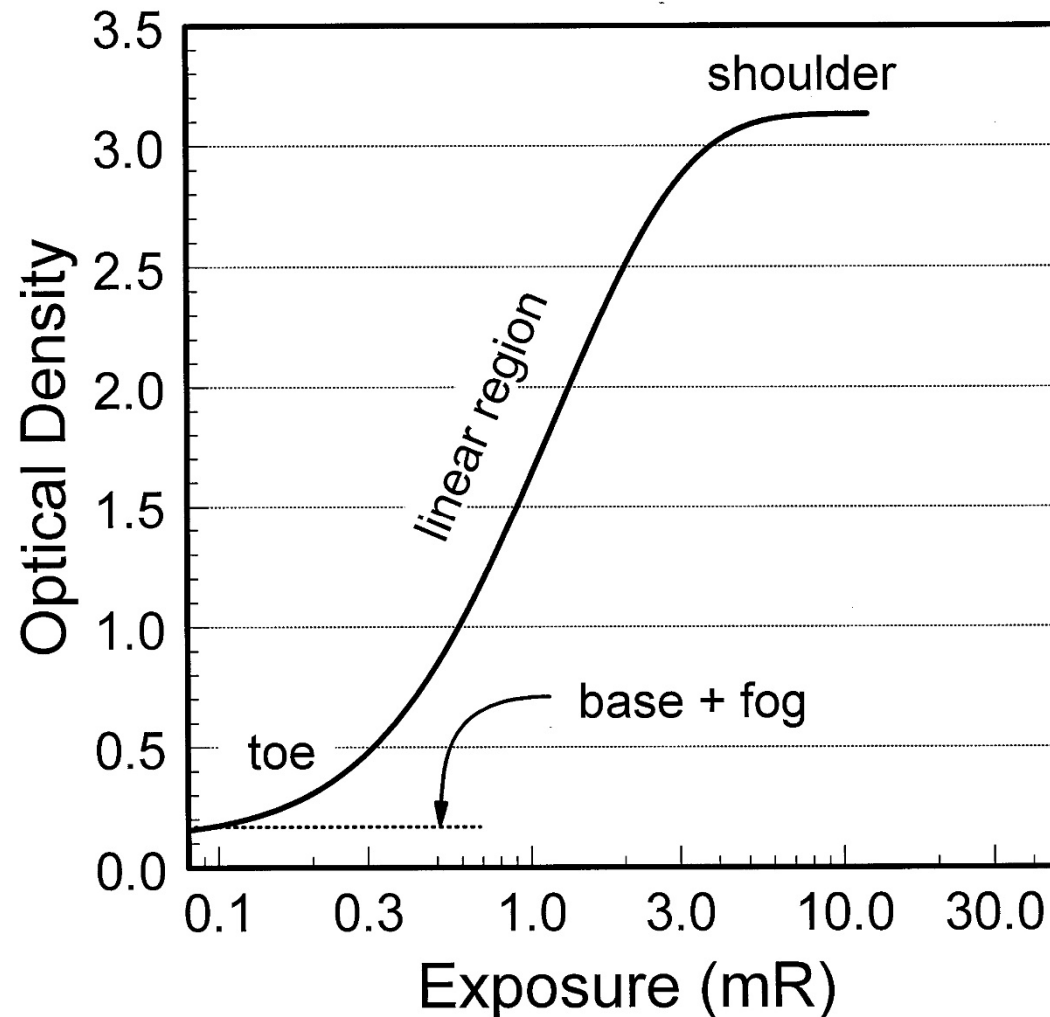






❖ **The characteristics curve of the film [Hurter and Driffield (H & D) curve]**

The film has a non-linear response to exposure



## 3.2 Geometry of Projection Radiography

- ❖ We must briefly consider some geometric factors that influence the quality of the x-ray image

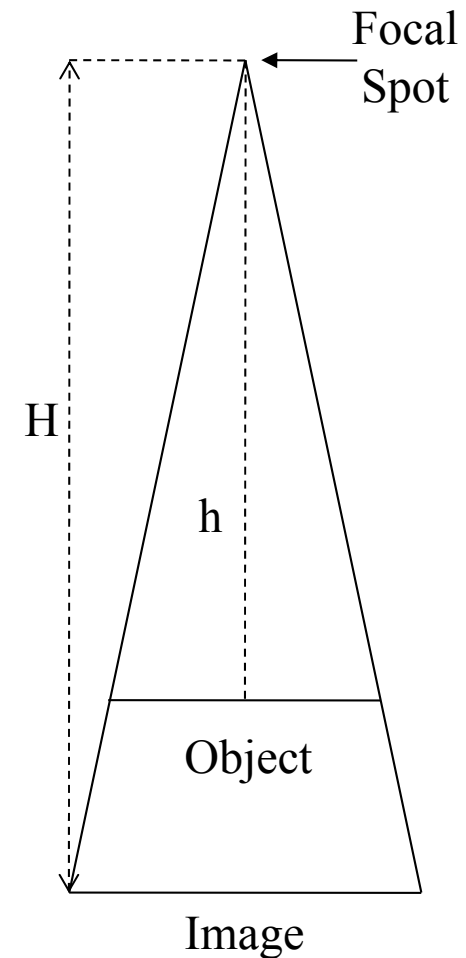
### (1) Magnification

$$\begin{aligned} M &= (\text{size of the image}) / (\text{size of the object}) \\ &= (\text{source-to-image detector distance}) \\ &\quad / (\text{source-to-object distance}) \\ &= H / h \end{aligned}$$

Under usual radiographic situations, magnification should be kept to a minimum.

Two rules apply:

- Keep the object as close to the film as possible,
- Keep the source-to-image detector distance as large as possible.



### Example:

A patient is placed so that a vertebral body and the sternum are 5cm and 25 cm from the cassette, respectively. The cassette is 100cm from the focal spot of the X-ray tube. By how much are the images of the vertebral body and the sternum magnified?

### Solution:

For vertebral body:  $H = 100\text{cm}$ ,  $h = 100 - 5 = 95 \text{ cm}$

$$M = 100 / 95 = 1.05$$

For sternum:  $H = 100\text{cm}$ ,  $h = 100 - 25 = 75 \text{ cm}$

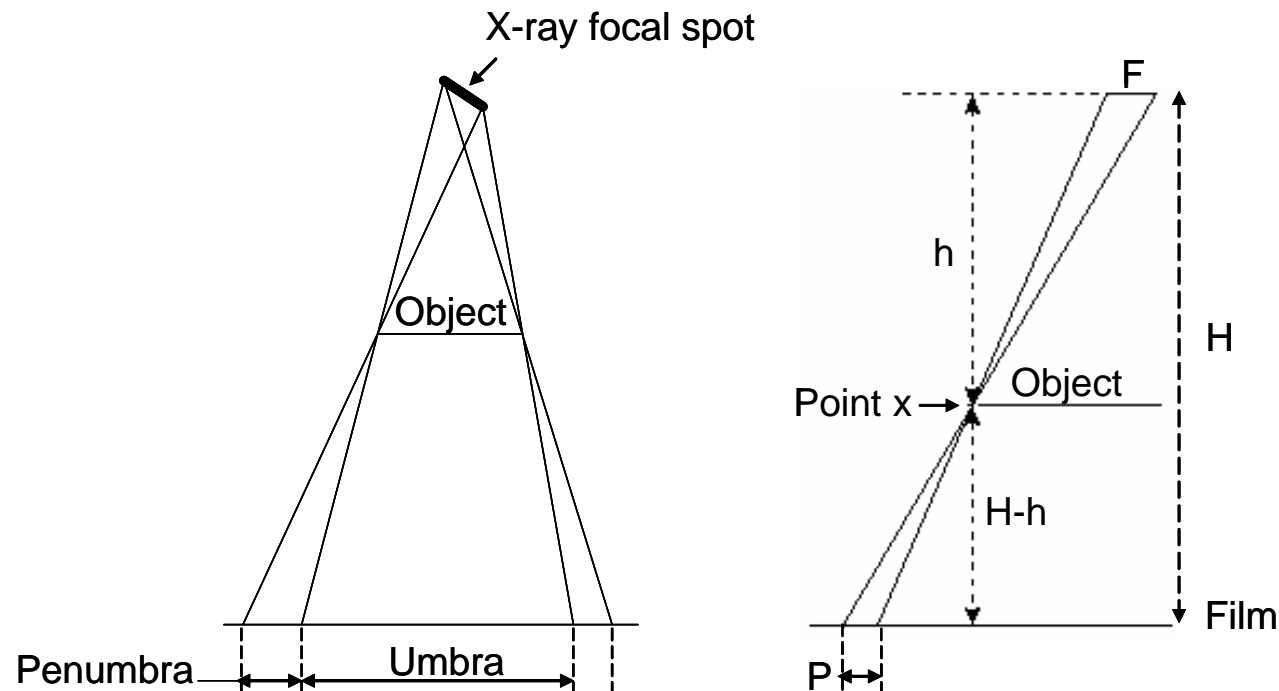
$$M = 100 / 75 = 1.33$$

Note: In clinical projection radiography, **M is always larger than 1.**

**(2) Penumbra** (from the latin *pene*, meaning almost and *umbra*, meaning shadow), also called geometric unsharpness, penumbra, or edge gradient, which is due to the fact that the x-ray source is not a perfect point source.

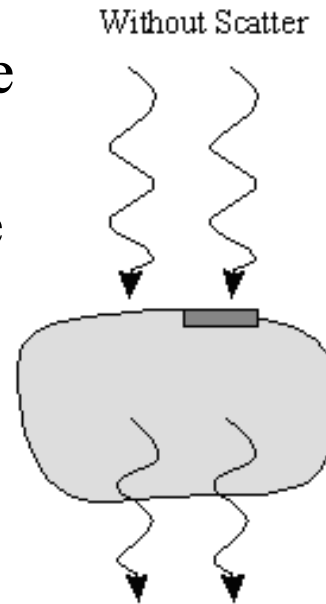
The width of penumbra  $P = F \frac{H - h}{h}$

- (a) Keep the object as close to the film as possible,
- (b) keep the source-to-image detector distance as large as possible.
- (c) Use as small as a focal spot as possible

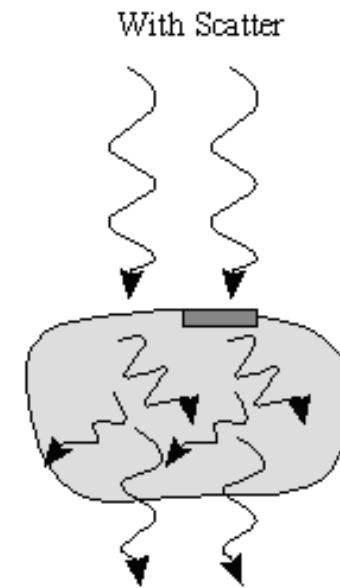


### 3.3 Scatter Control

- ❖ X-ray scatter decrease the contrast
- ❖ X-ray scatter increase the noise



$$C = \frac{N_b - N_l}{N_b}$$



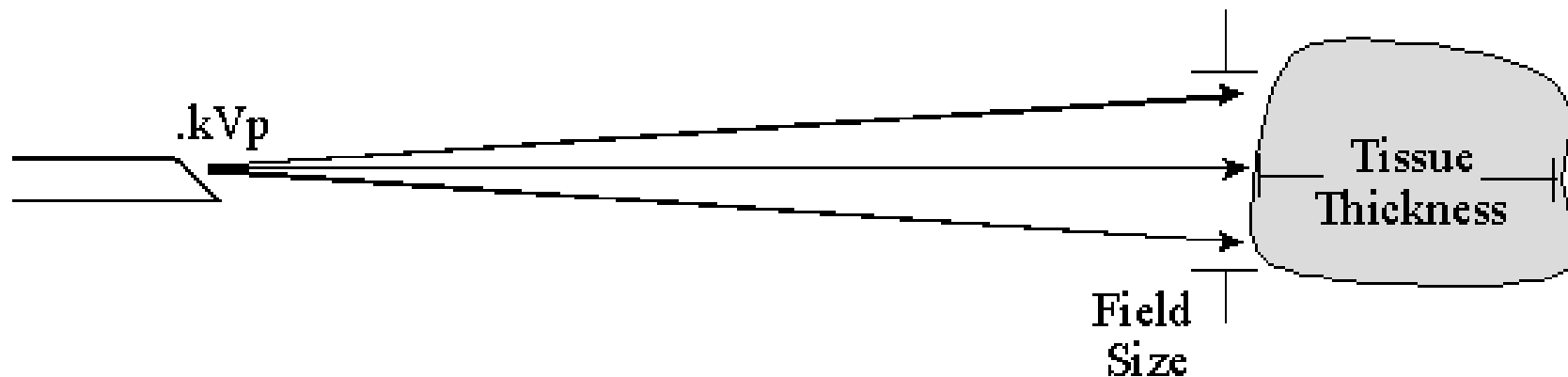
$$C' = \frac{N_b - N_l}{N_b + S}$$

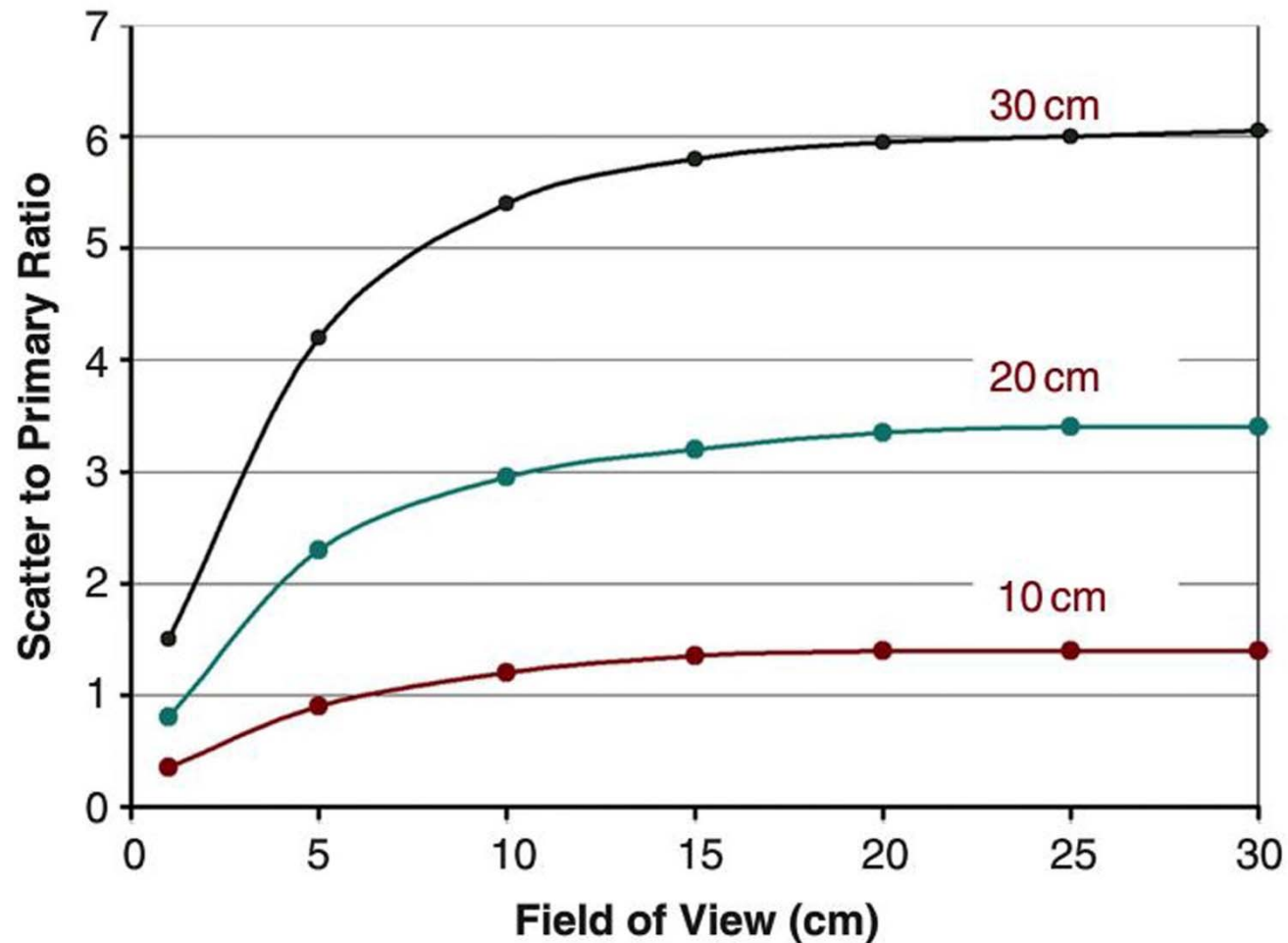
$$\begin{aligned} &= \frac{\frac{N_b - N_l}{N_b}}{1 + \frac{S}{N_b}} = \frac{1}{1 + \frac{S}{N_b}} C \\ &= \frac{1}{1 + \frac{S}{P}} C \end{aligned}$$

In the above equation, S/P is called  
**Scatter to Primary Ratio**

❖ The following factors may affect the amount of scatter:

- Radiation field size (smaller field size, less scatter);
- Patient thickness (less thickness, less scatter);

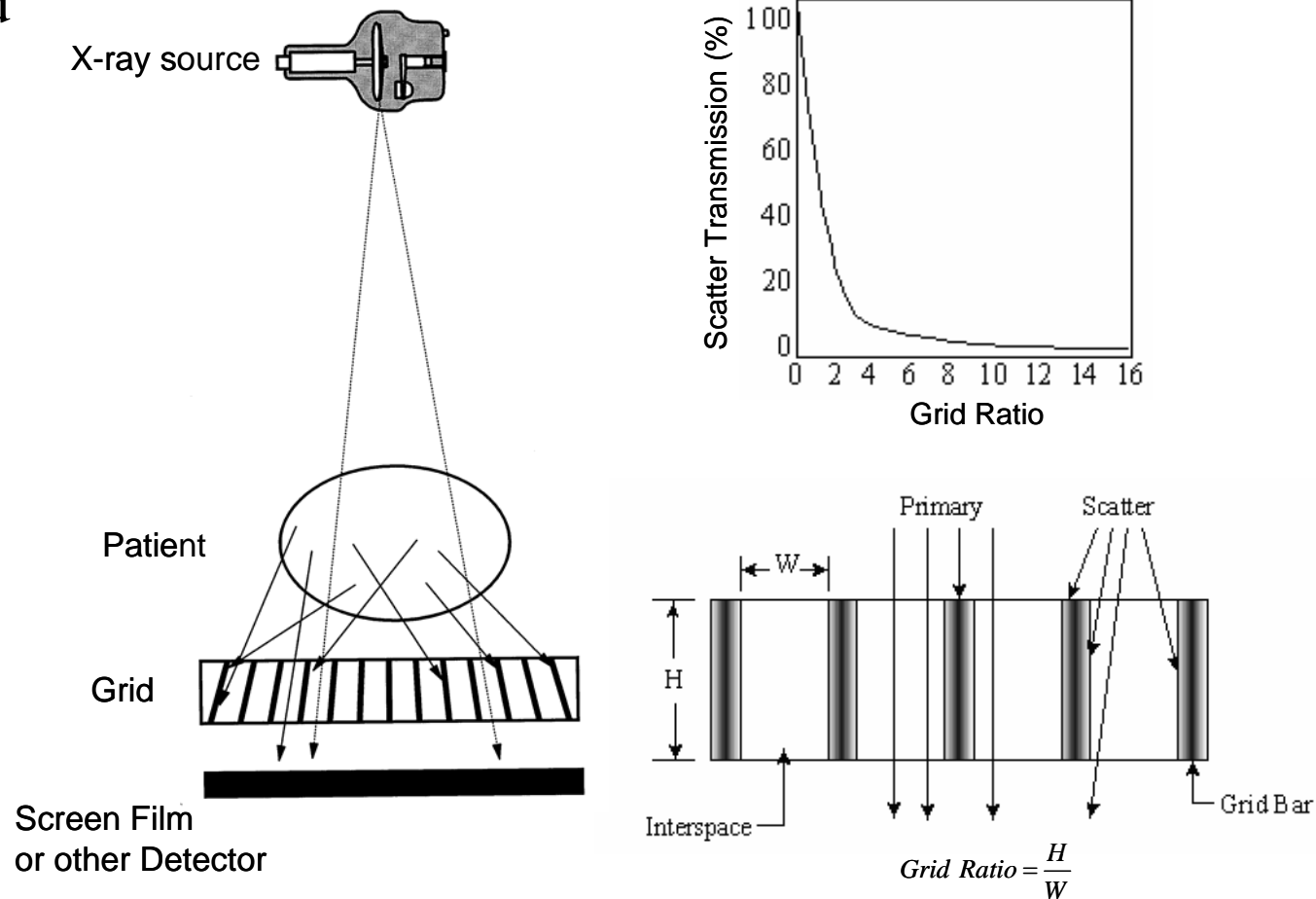




**Figure** The S/P is shown as a function of the side dimension of a square field of view, for three different patient thicknesses. The S/P increases with increasing field size and with increasing patient thickness. Thus, scatter is much more of a problem in the abdomen as compared to extremity radiography. Scatter can be reduced by aggressive use of collimation, which reduces the field of view of the x-ray beam. (Page231, The Essential Physics of Medical Imaging, Third Edition)

# Methods to reduce scattered radiation

## (a) Grid



**Grid Ratio:** The **Grid Ratio** is determined by the **height** of the grid bars divided by the **width** of the **interspace** material

$$\text{Grid Ratio} = \frac{H}{W}$$



- ❖ When Grid is used, the contrast is improved, the following table is an example\*

<b>Grid Ratio</b>	<b>No Grid</b>	<b>2:1</b>	<b>4:1</b>	<b>8:1</b>	<b>12:1</b>	<b>16:1</b>
<b>Relative Contrast* (70KVp)</b>	1	2	3	4.8	5.3	5.8
<b>Relative Contrast* (95KVp)</b>	1	1.5	2.0	3.3	3.8	4.0
<b>Relative Contrast* (120KVp)</b>	1	1.3	1.5	2.5	3.0	3.3

\*Contrast relative to that with no Grid, using a 20cm thick water phantom and a test pattern.

- National Council on Radiation Protection and Measurements (NCRP): Medical X-ray, Electron Beam and Gamma-Ray Protection for energies up to 50MeV (equipment Design), Performance, and Use (Report No 102). Bethesda, MD NCRP, 1989 (Table B.4)

- ❖ When a grid is used, the x-ray exposure to the patient has to be increased (so the exposure to the detector remains the same with and without grid).
- ❖ The **Bucky factor** is a measure of the ratio in incident exposure to the patient, with and without the grid.

Another way to describe the Bucky factor:

**Bucky factor** = (the total exposure incident to the grid) /  
(the total exposure transmitted through the  
grid)

The following table is an example of **Bucky** factors under certain conditions

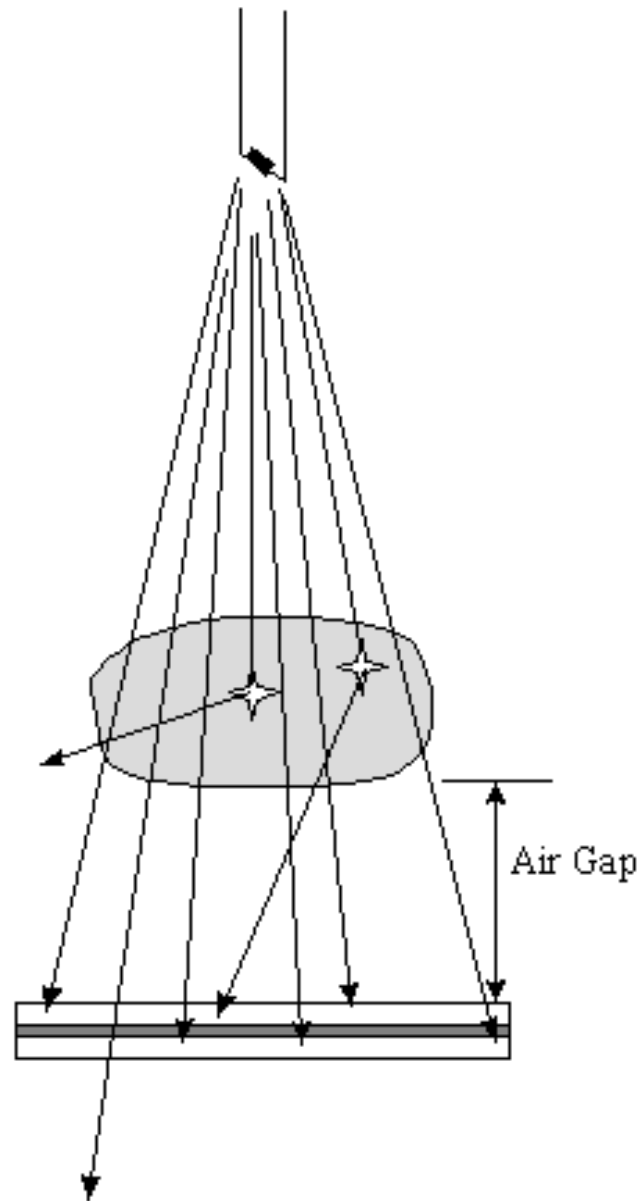
<b>Grid Ratio</b>	<b>No Grid</b>	<b>2:1</b>	<b>4:1</b>	<b>8:1</b>	<b>12:1</b>	<b>16:1</b>
<b>Bucky factor (70KV<sub>p</sub>)</b>	1	1.1	2.7	3.5	4.0	4.5
<b>Bucky factor (95KV<sub>p</sub>)</b>	1	1.1	2.7	3.8	4.3	5.0
<b>Bucky factor (120KV<sub>p</sub>)</b>	1	1.1	2.7	4.0	5.0	6.0

- National Council on Radiation Protection and Measurements (NCRP): Medical X-ray, Electron Beam and Gamma-Ray Protection for energies up to 50MeV (equipment Design), Performance, and Use (Report No 102). Bethesda, MD NCRP, 1989 (Table B.4)

## **Discussions:**

- ❖ Why one has to increase the x-ray exposure to the patient when a grid is used ?
- ❖ The grid has to be moved back and forth during the x-ray exposure, why?

(b) Air gap



## SUMMARY

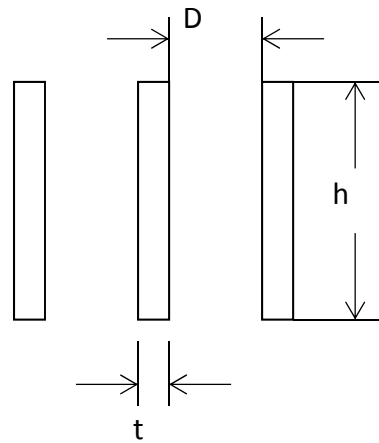
- ❖ The **intensification factor** = (X-ray exposure required without screen) / (x-ray exposure required with screen)
- ❖ The film has a **nonlinear** response to exposure
- ❖ **Penumbra:**
  - (i) Keep the object as close to the film as possible,
  - (ii) keep the source-to-image detector distance as large as possible.
  - (iii) Use as small as a focal spot as possible
- ❖ **Scatter to primary ratio : (S/P)**
  - (i) Radiation field size (smaller field size, less scatter);
  - (ii) Patient thickness (less thickness, less scatter);
- ❖ **Grid**

Grid ratio: the **height** of the grid bars divided by the width of the **interspace** material
- ❖ **Bucky factor:** a measure of the ratio in incident exposure to the patient, **with** and **without** the grid.
- ❖ **Air gap:** larger the air gap, less the scatter

## Homework # 3

1. What is a radiographic penumbra? (Draw a simple picture to illustrate), and what causes it ?
2. What is the "intensification factor" of a screen?
3. Assume that 1000 x-ray photons, each with an energy of 100 keV, are incident on a intensifying screen with an absorption efficiency (quantum efficiency) of 50% and an intrinsic efficiency of 20%.
  - (a) How many x-rays photons will contribute to the image?
  - (b) Assuming the average energy of a blue light photon is 3eV, how many blue light photons will be produced for each x-ray photon absorbed?

4. If a screen is made thicker, what happens to the spatial resolution?
5. A linear scatter grid has dimensions shown here, where  $D$  is 0.1mm and  $h$  is 0.2mm. What is the grid ratio?



6. If the grid ratio is doubled, does the number of scattered x-rays contributing to the image increase or decrease? \_\_\_\_\_.