

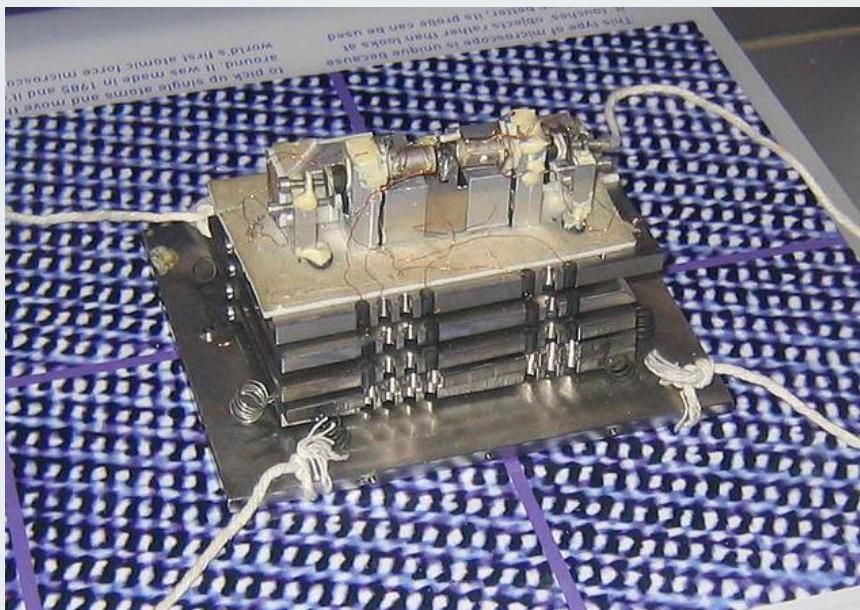


**qbio**  
quantitative  
biology

# Atomic Force Microscopy and Scanning Probe Microscopy



1981 - Invention of the STM



1986 - Invention of the AFM

The Nobel Prize in Physics 1986  
Ernst Ruska, Gerd Binnig, Heinrich Rohrer

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## The Nobel Prize in Physics 1986



Ernst Ruska  
Prize share: 1/2



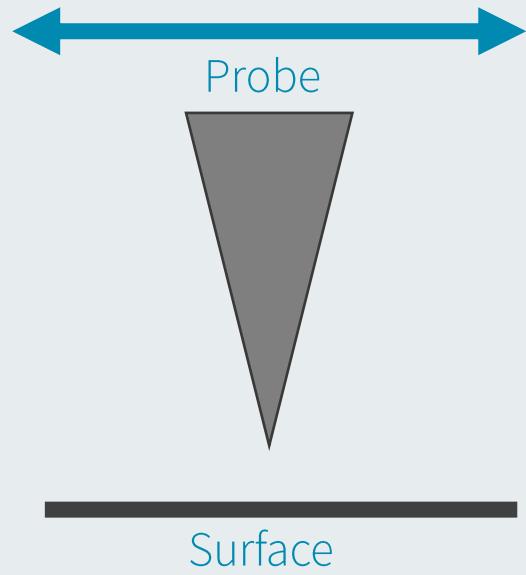
Gerd Binnig  
Prize share: 1/4



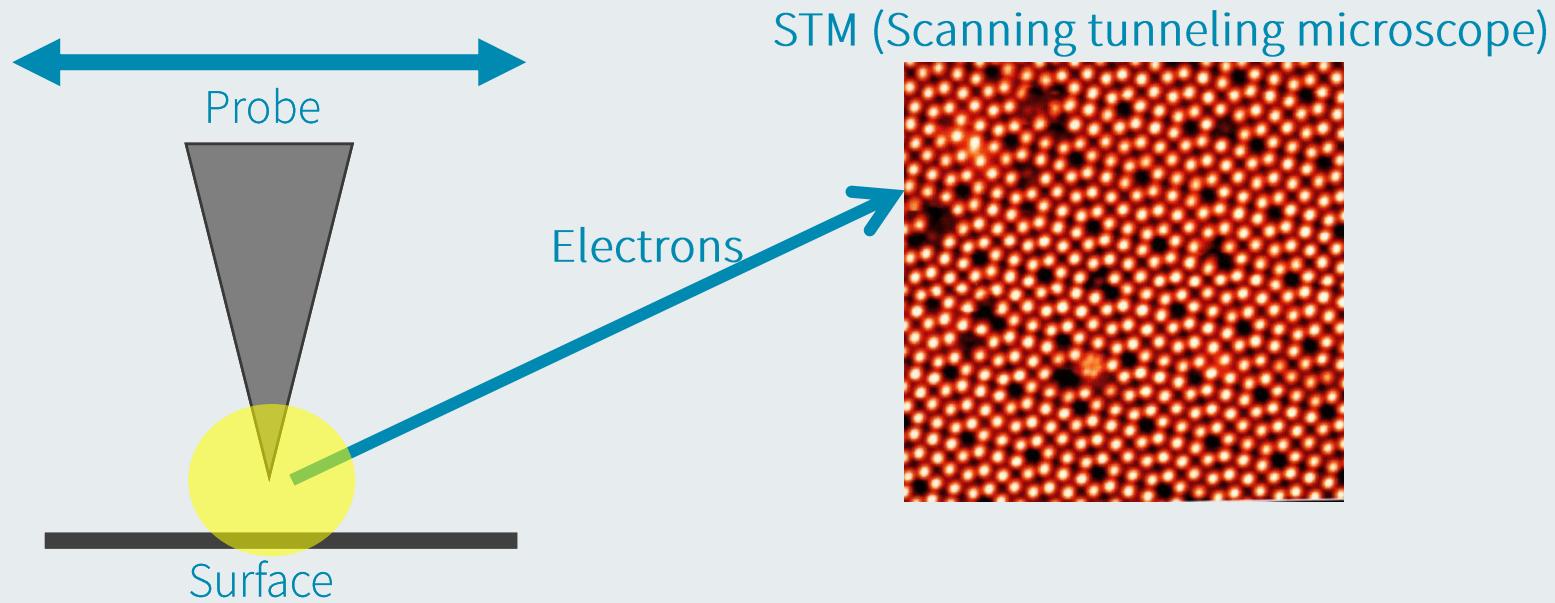
Heinrich Rohrer  
Prize share: 1/4

Binnig G, Quate CF, Gerber C. Atomic force microscope. *Phys. Rev. Lett.* 1986 Mar 3;56(9):930-933

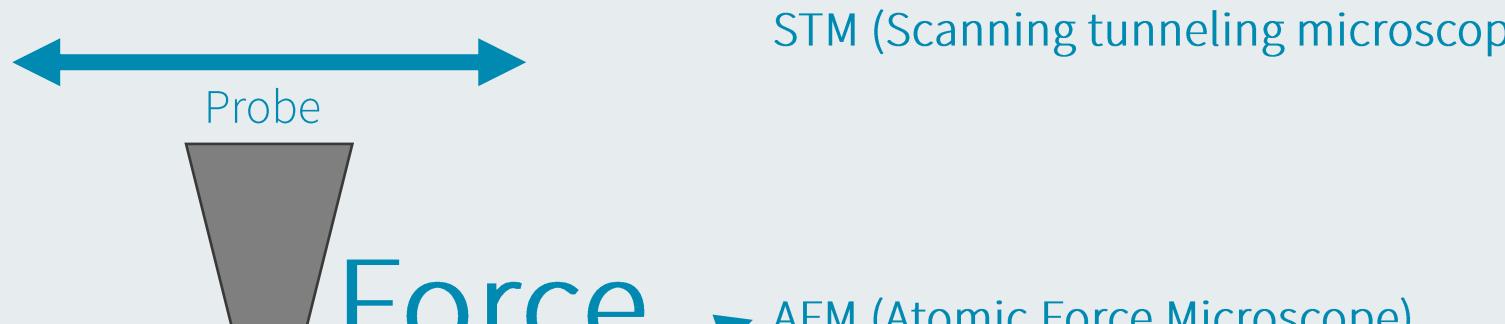
# Atomic Force Microscopy and Scanning Probe Microscopy



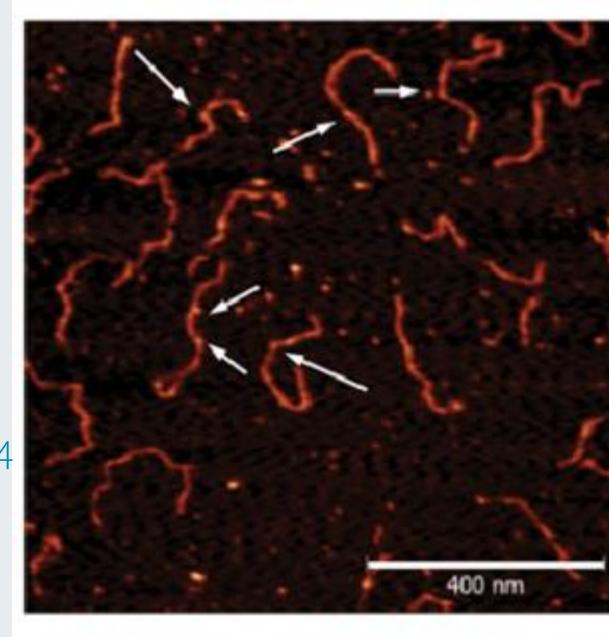
# Atomic Force Microscopy and Scanning Probe Microscopy



# Atomic Force Microscopy and Scanning Probe Microscopy



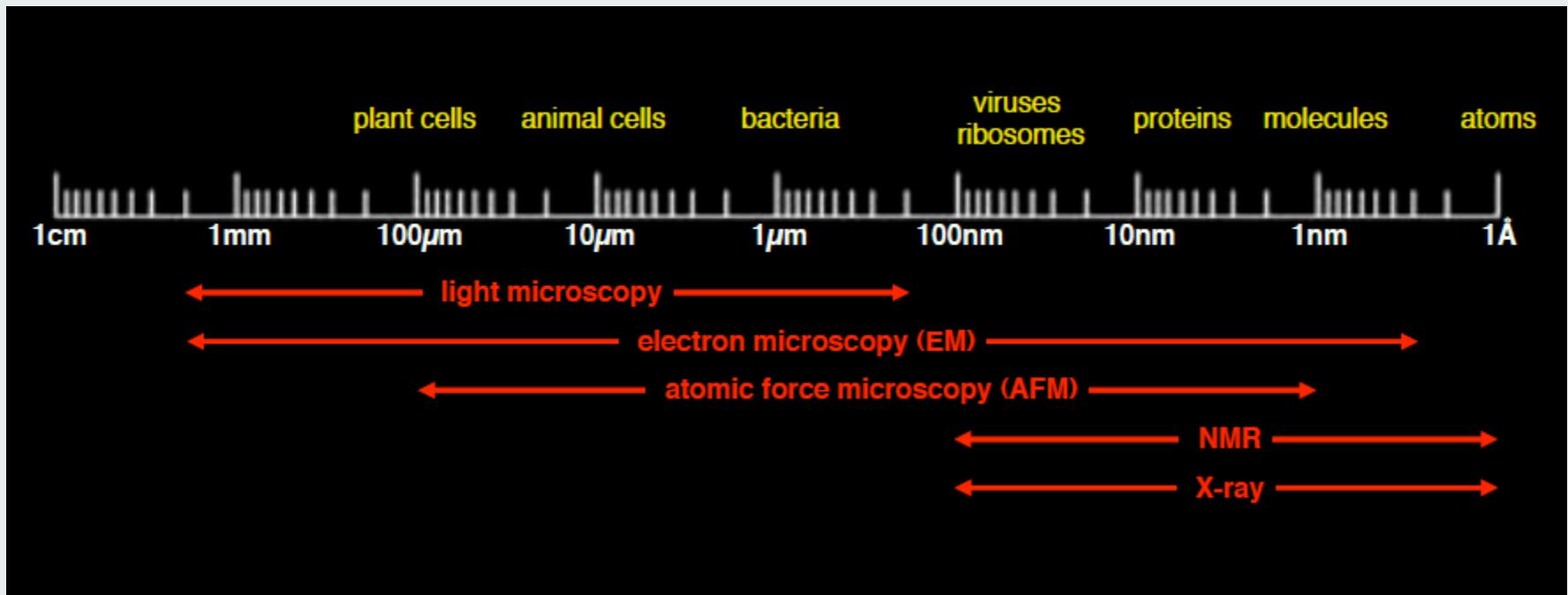
Puranik et al. *Plant Cell*, 2014



# Techniques in Structural Biology



Dimensions in life science – what technique is appropriate

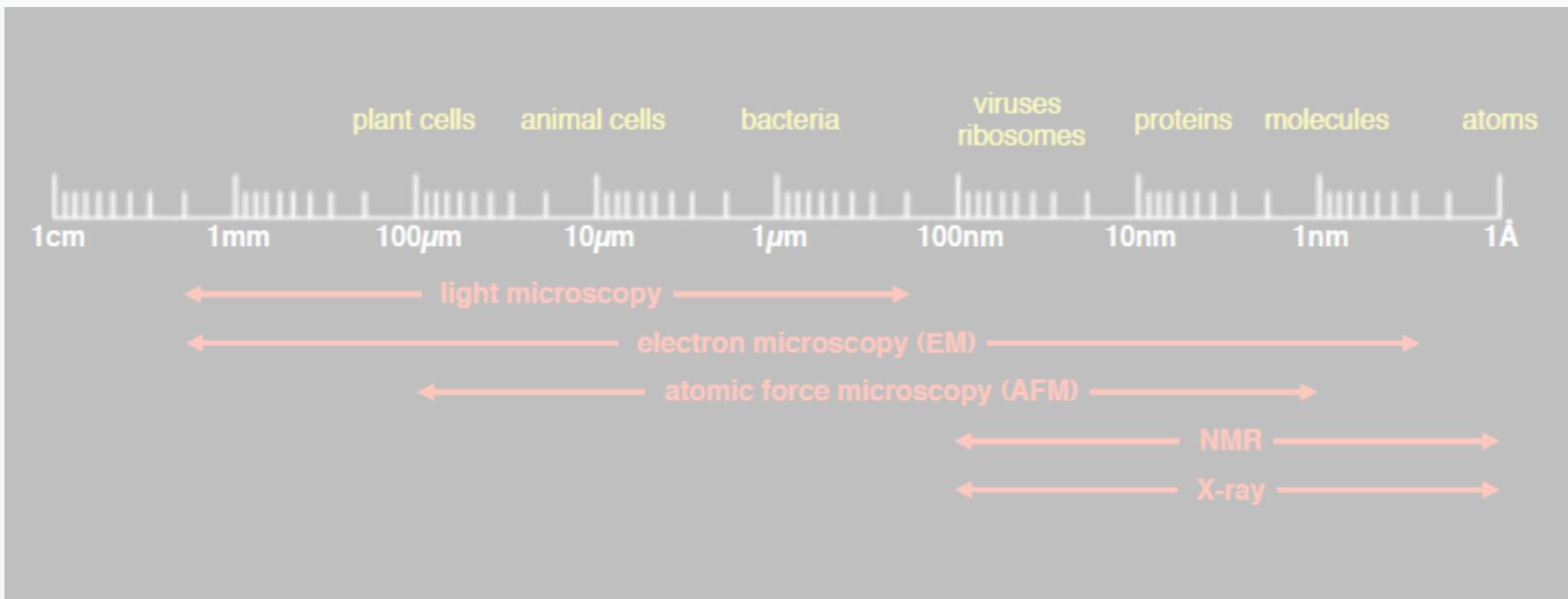


S. Scheuring, AFMBioMed Summer School, Marcoule 2011

# Techniques in Structural Biology



Dimensions in life science – what technique is appropriate

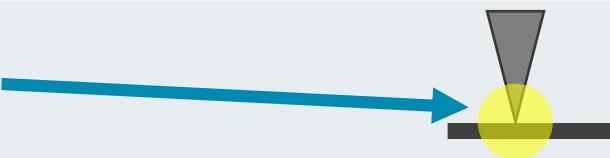


S. Scheuring, AFMBioMed Summer School, Marcoule 2011

LENGTHSCALE  
TIMESCALE

1) Introduction to Scanning Probe Microscopy

2) The Force



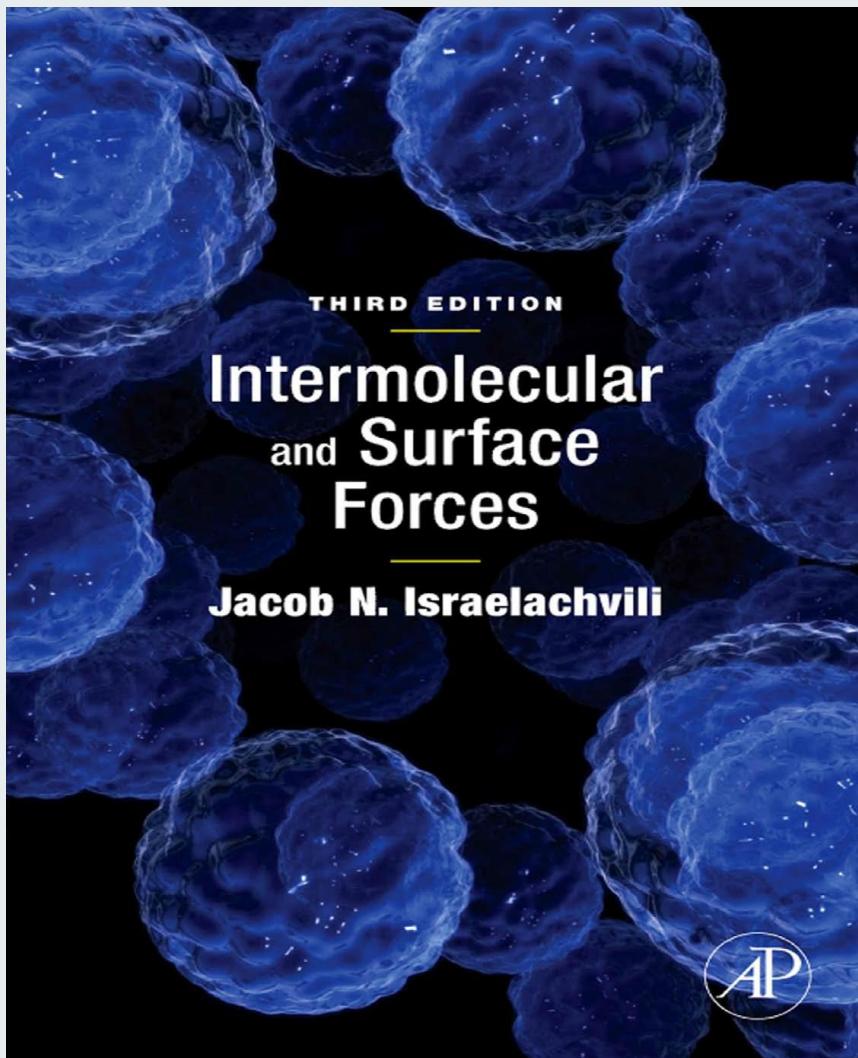
3) Methods

Cantilevers

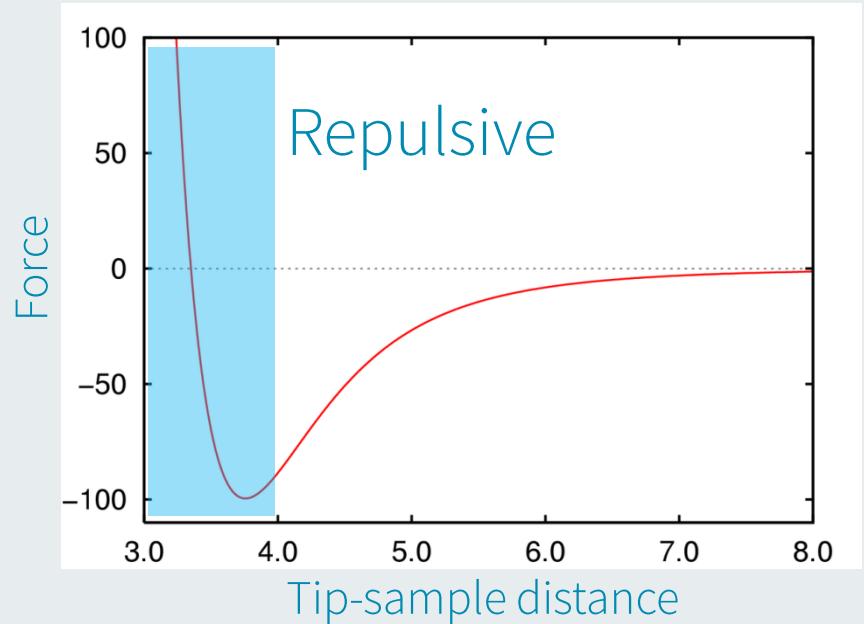
Static and Dynamic AFM

4) Instruments

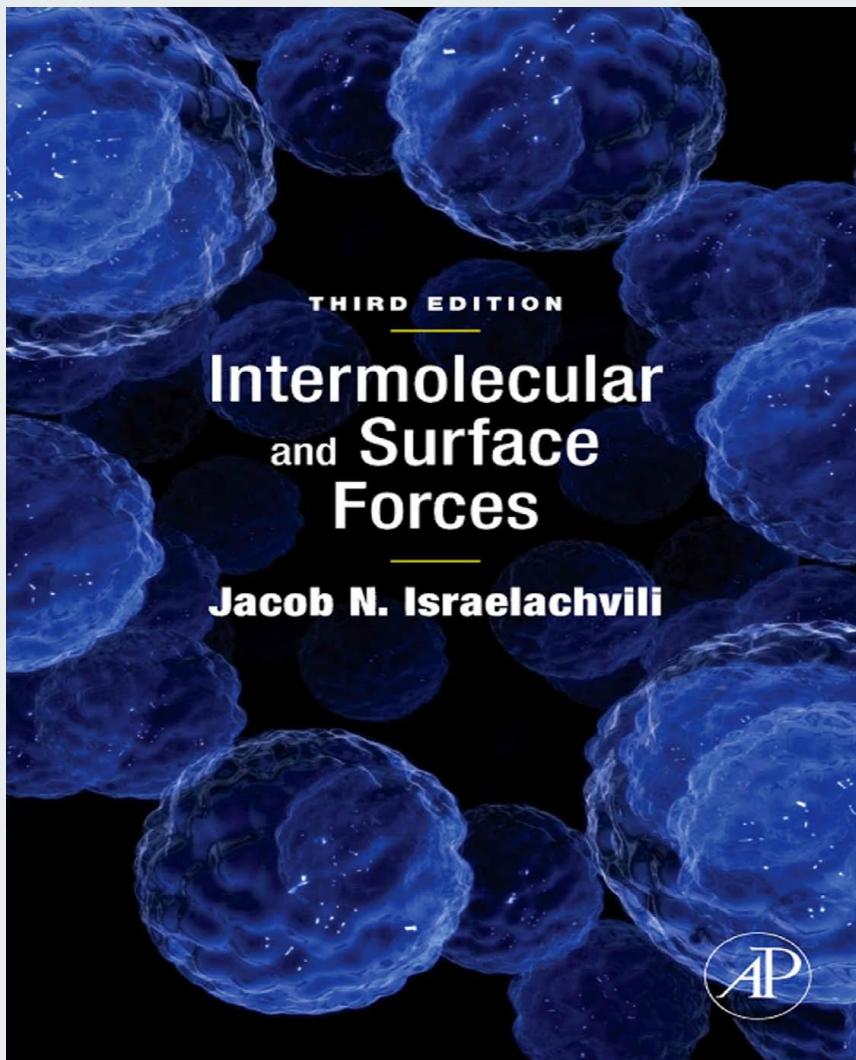
5) Advanced and novel AFM methods



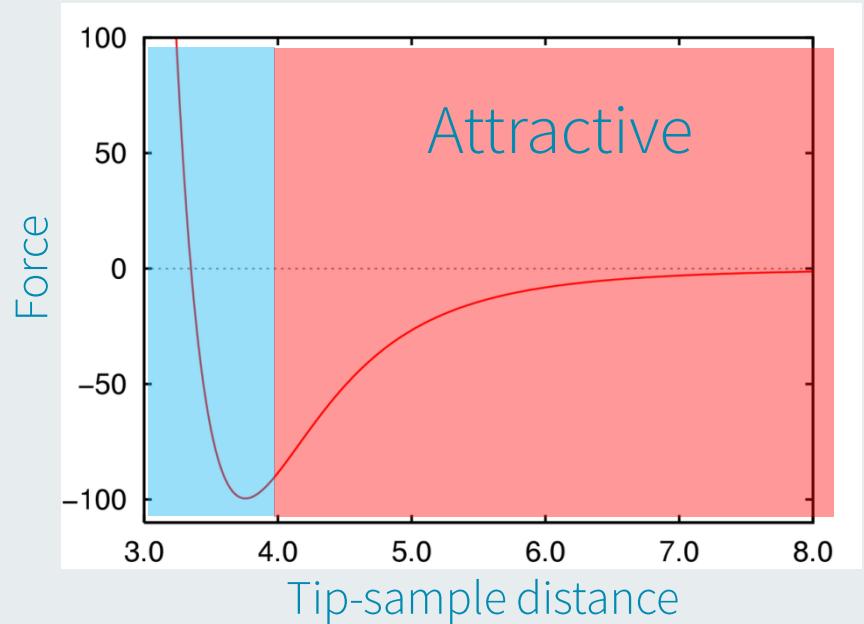
# Force



Repulsion due to overlap of  
tip-sample  
electronic shells



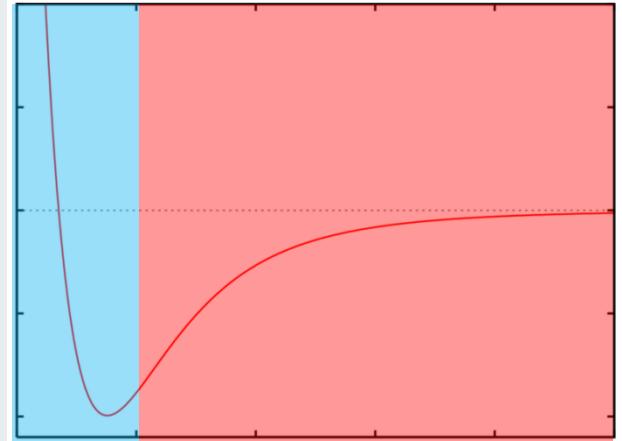
# Force



Attraction due to  
Van der Waals, capillarity....

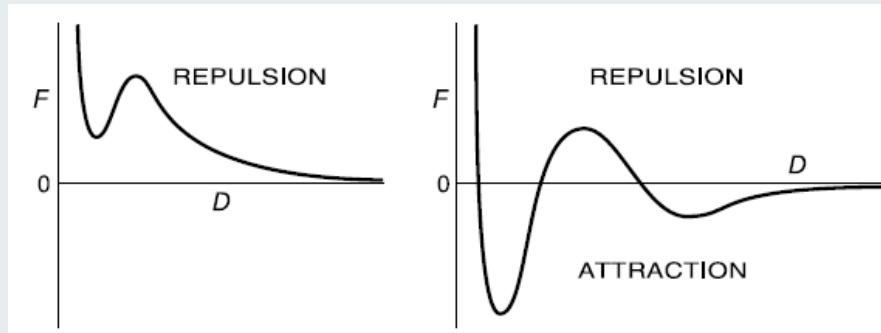


Richard P.  
Feynman  
(1918 – 1988)



*“...If, in some cataclysm, all of scientific knowledge were to be destroyed, and only one sentence passed on to the next generations of creatures, what statement would contain the most information in the fewest words? I believe it is the atomic hypothesis (or the atomic fact, or whatever you wish to call it) that all things are made of atoms—little particles that move around in perpetual motion, attracting each other when they are a little distance apart, but repelling upon being squeezed into one another...”*

# Interaction Forces at nanoscale



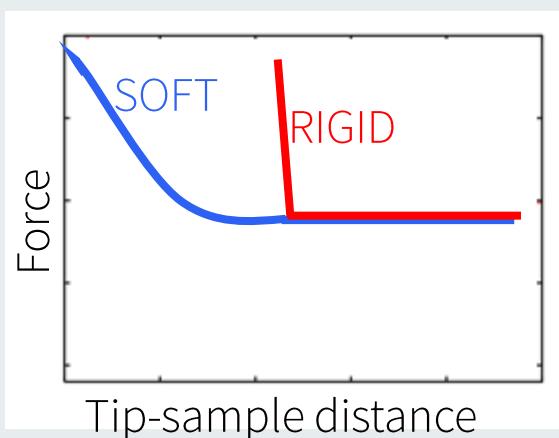
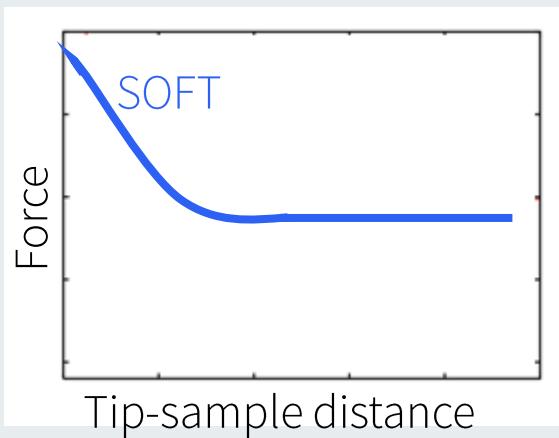
Tip sample Interaction Force depends on

- 1) Tip and sample geometry
- 2) Tip and sample nature (chemical affinity, charges)
- 3) Tip and/or Sample stiffness
- 4) Environment (liquid, air, gas, vacuum)

# Interaction Forces at nanoscale



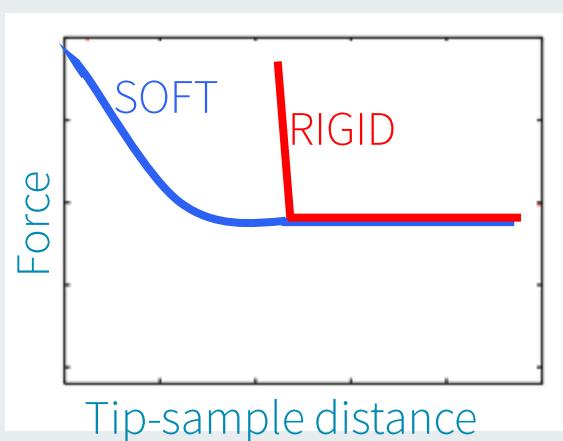
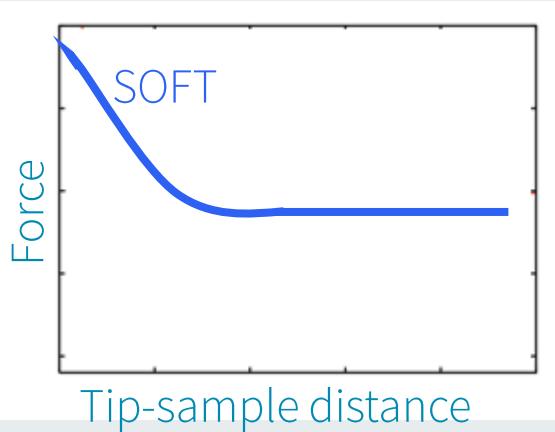
Tip and/or Sample stiffness



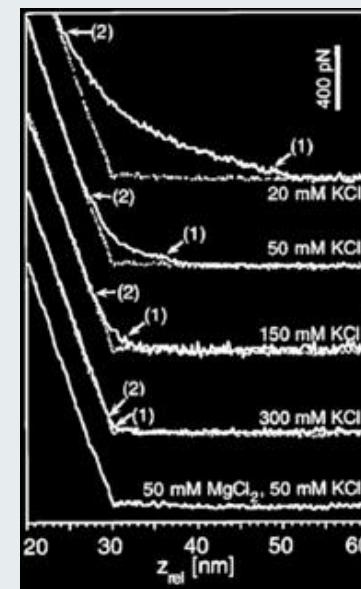
# Interaction Forces at nanoscale



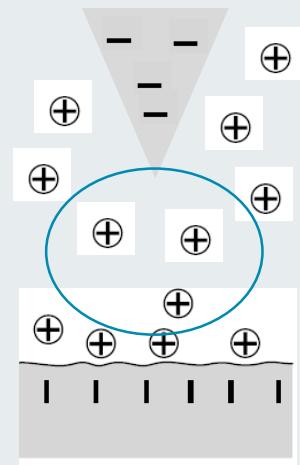
Tip and/or Sample stiffness



Environment: liquid + salt



IONS ARE  
IMPORTANT!!!



Daniel J Müller, Dimitrios Fotiadis, Simon Scheuring, Shirley A Müller & Andreas Engel *Electrostatically balanced subnanometer imaging of biological specimens by atomic force microscopy* *Biophys J*, 1999, 76 (2): 1101-1111

1) Introduction to Scanning Probe Microscopy

2) The Force



3) Methods

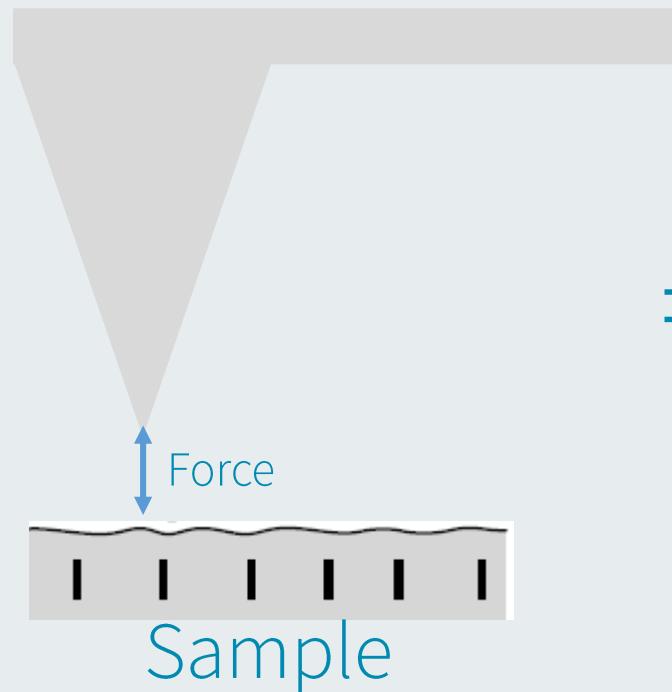
Cantilevers

Static and Dynamic AFM

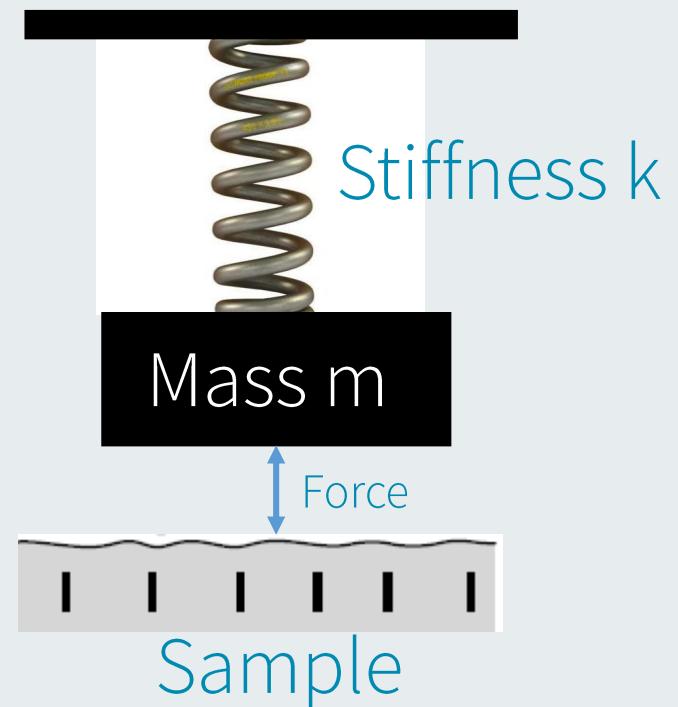
4) Instruments

5) Advanced and novel AFM methods

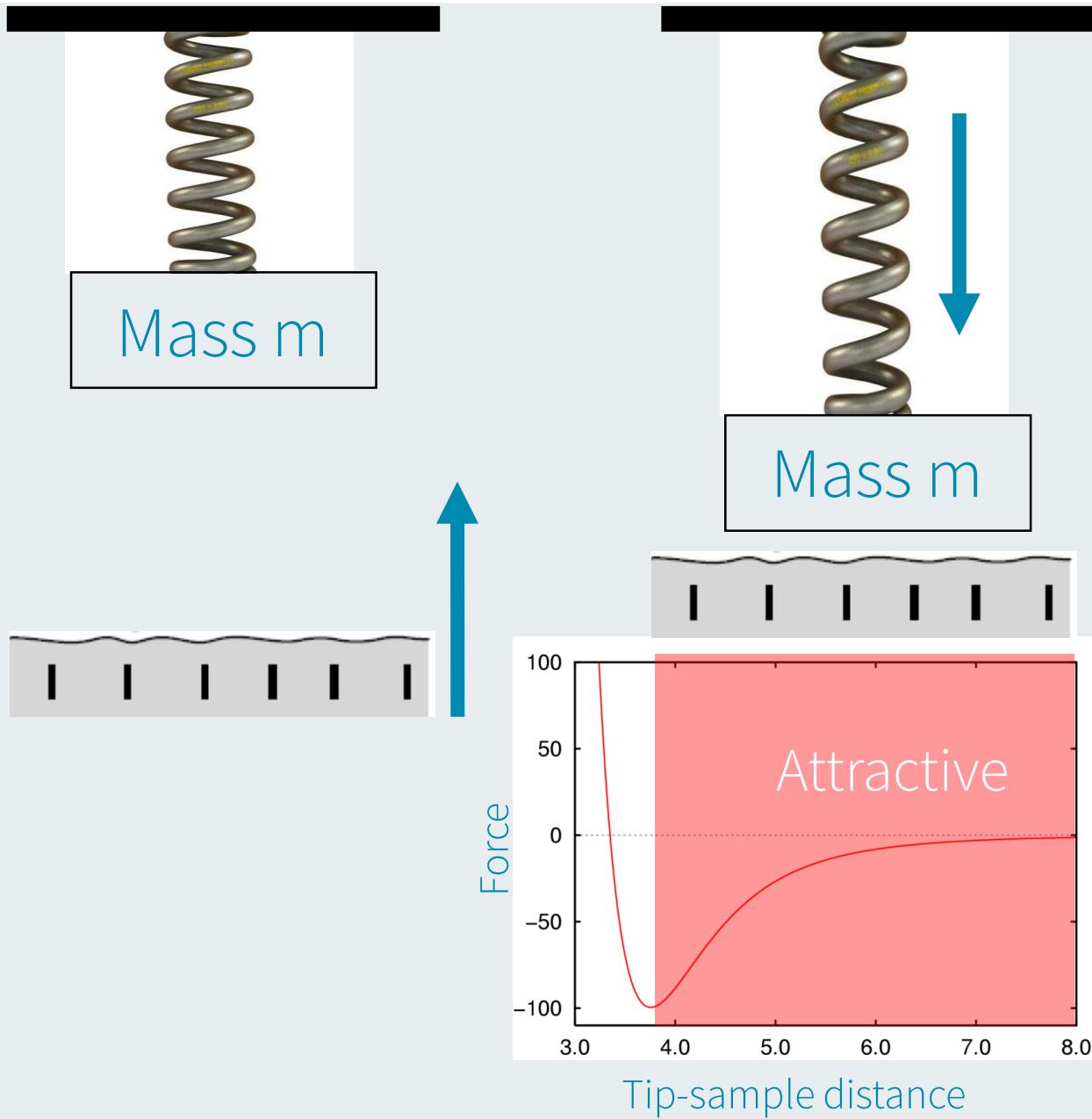
Cantilever



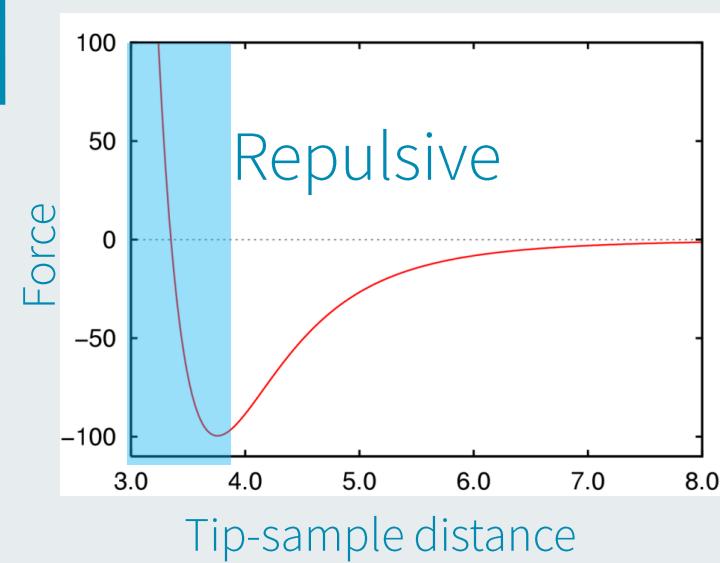
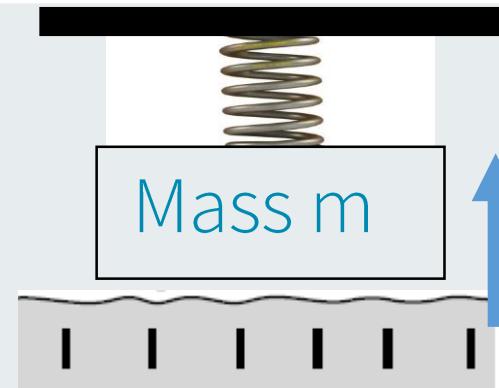
=



# Cantilevers

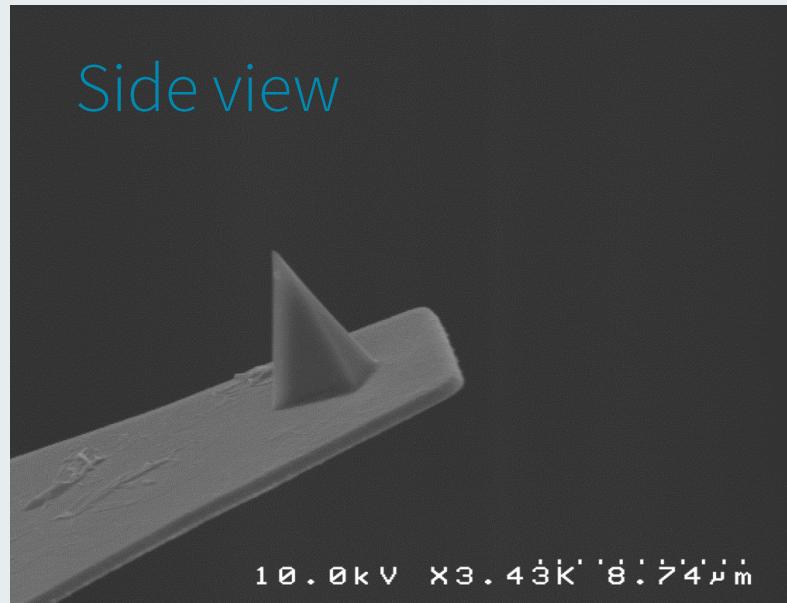
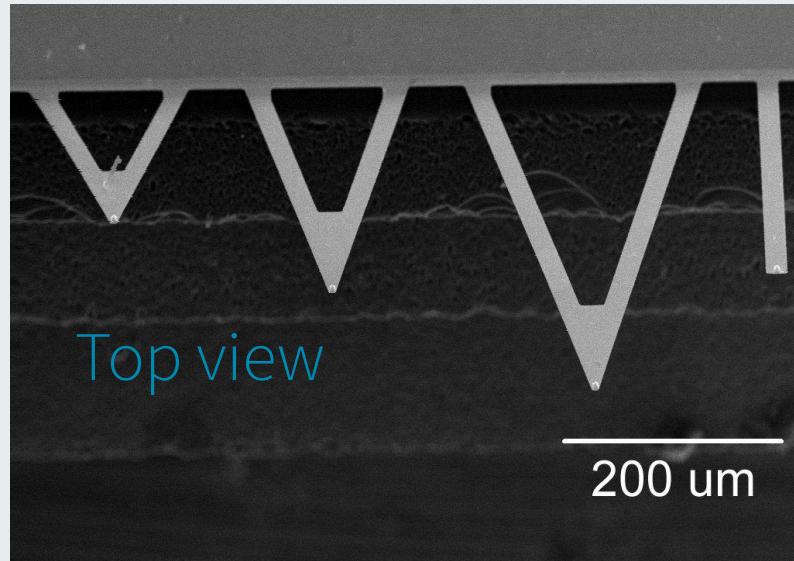
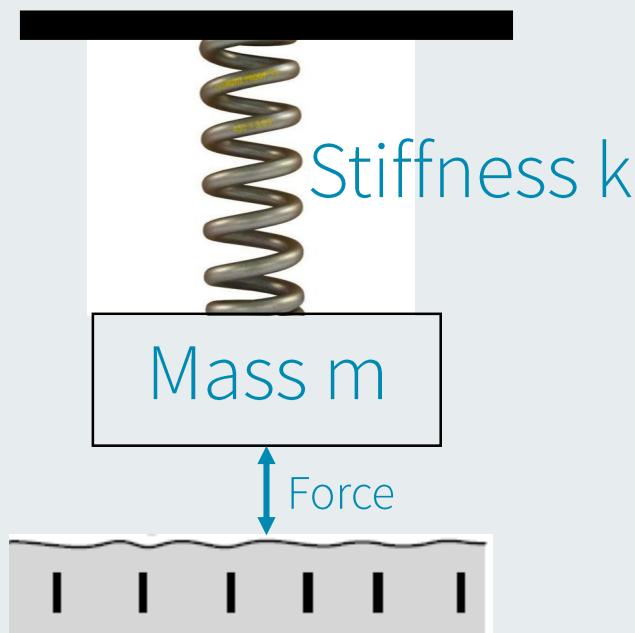


# Cantilevers



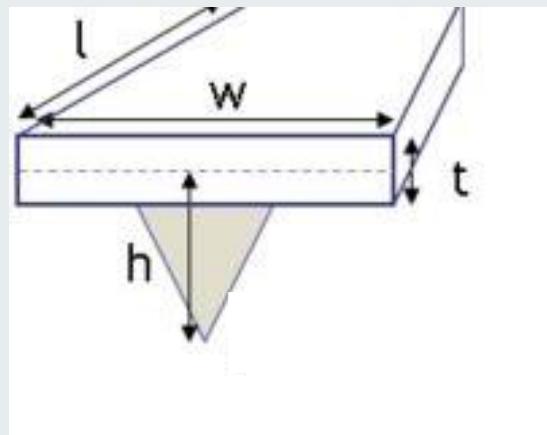
Tip-sample distance

# Cantilevers





Stiffness  $k$ : from 0.006 N/m to 100 N/m  
Extrinsic property



$$k = \frac{Ewt^3}{4L^3} \quad k \text{ must be calibrated !!}$$

$E$  = Young's modulus [Pa] intrinsic property

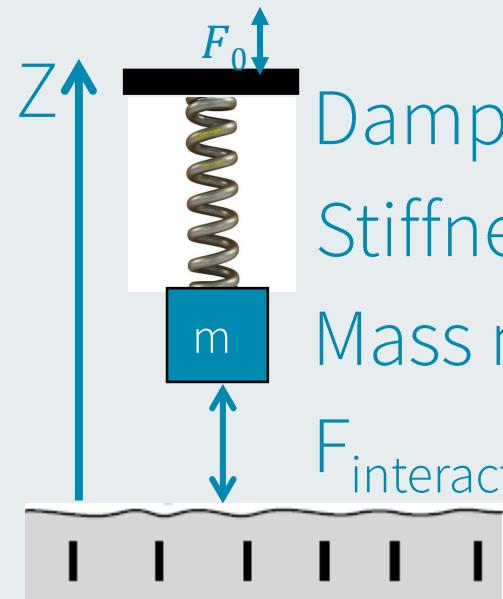
Length  $L$ : from 10  $\mu\text{m}$  to 500  $\mu\text{m}$

Materials: Silicon and Silicon Nitride

# Cantilevers and harmonic oscillators



$$m\ddot{z} + \delta\dot{z} + kz = F_{interaction}(z) + F_0(\omega t)$$



Damping  $\delta$  [N s /m]: environment, viscosity

Stiffness  $k$  [N/m]

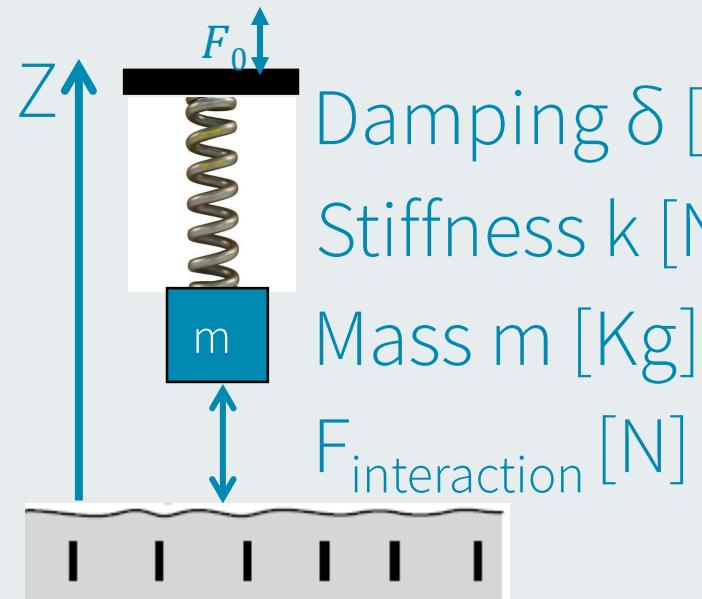
Mass  $m$  [Kg]

$F_{interaction}$  [N]

# Cantilevers and harmonic oscillators



$$m\ddot{z} + \delta\dot{z} + kz = F_{interaction}(z) + F_0(\omega t)$$



Damping  $\delta$  [N s /m]: environment, viscosity

Stiffness  $k$  [N/m]

Mass  $m$  [Kg]

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# Static AFM mode (contact mode)



STATIC AFM: tip in permanent contact with the sample



# Static AFM mode (contact mode)



STATIC AFM: tip in permanent contact with the sample



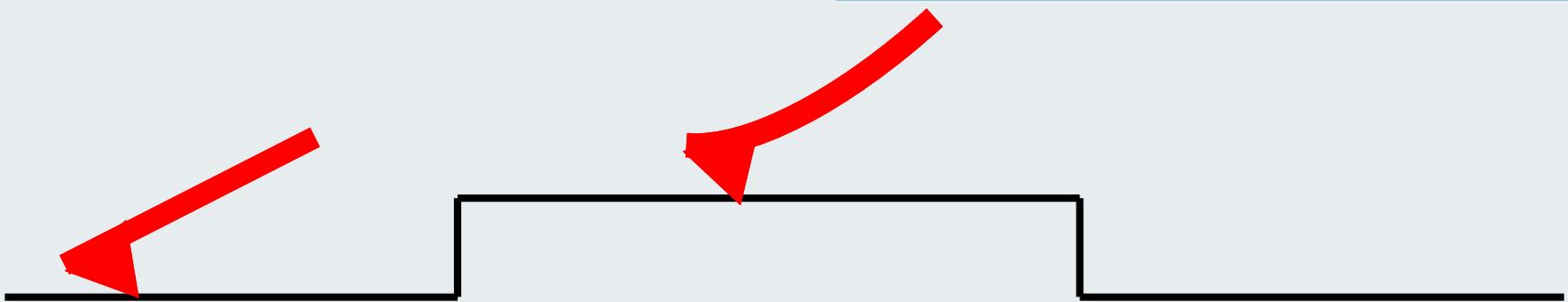
Phonograph



# Static AFM mode (contact mode)



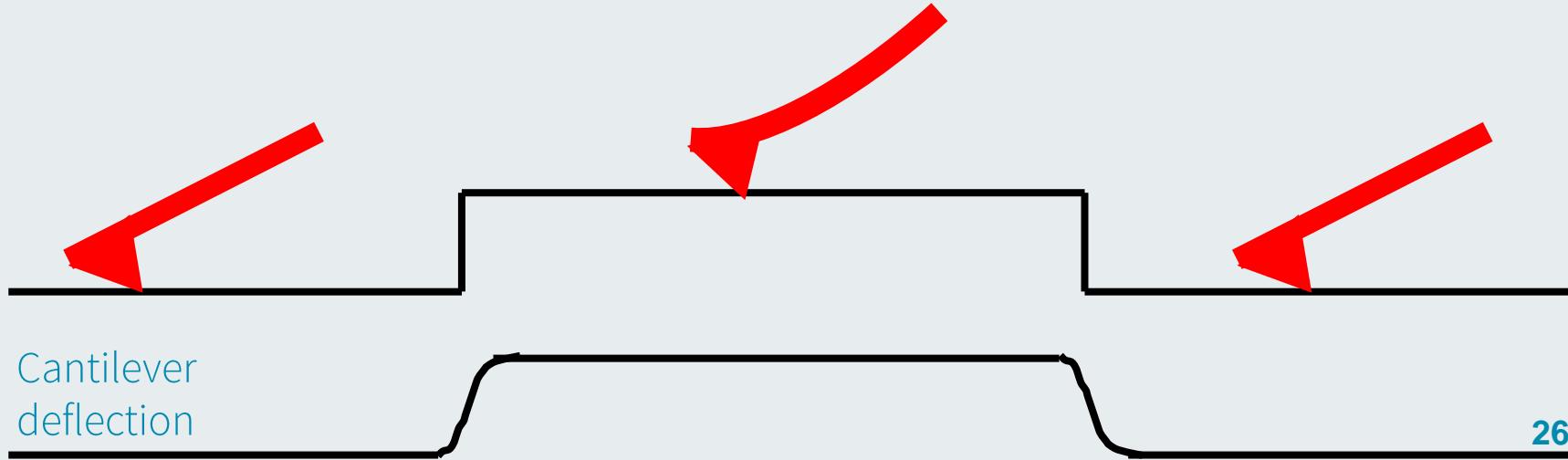
STATIC AFM: tip in permanent contact with the sample



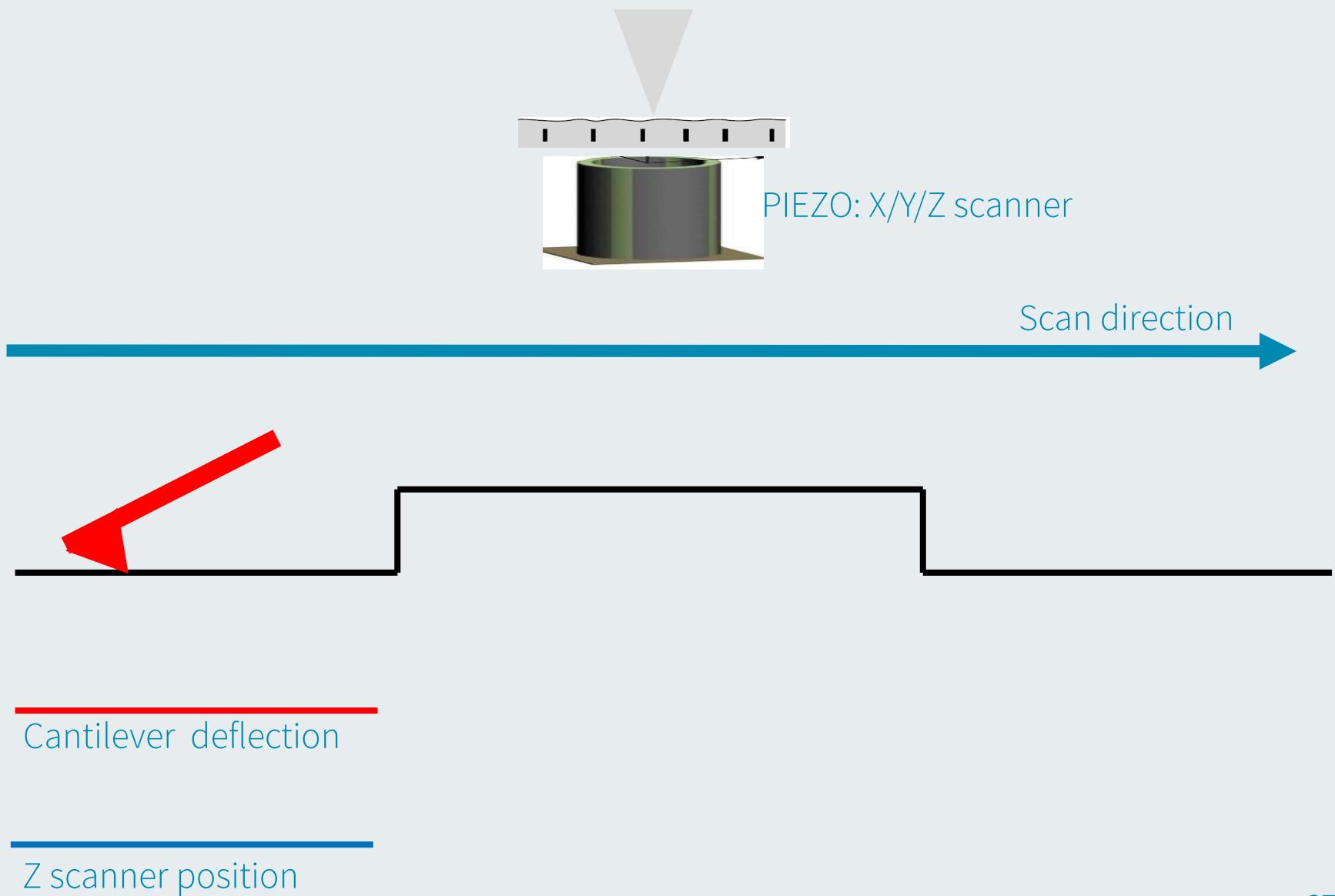
# Static AFM mode (contact mode)



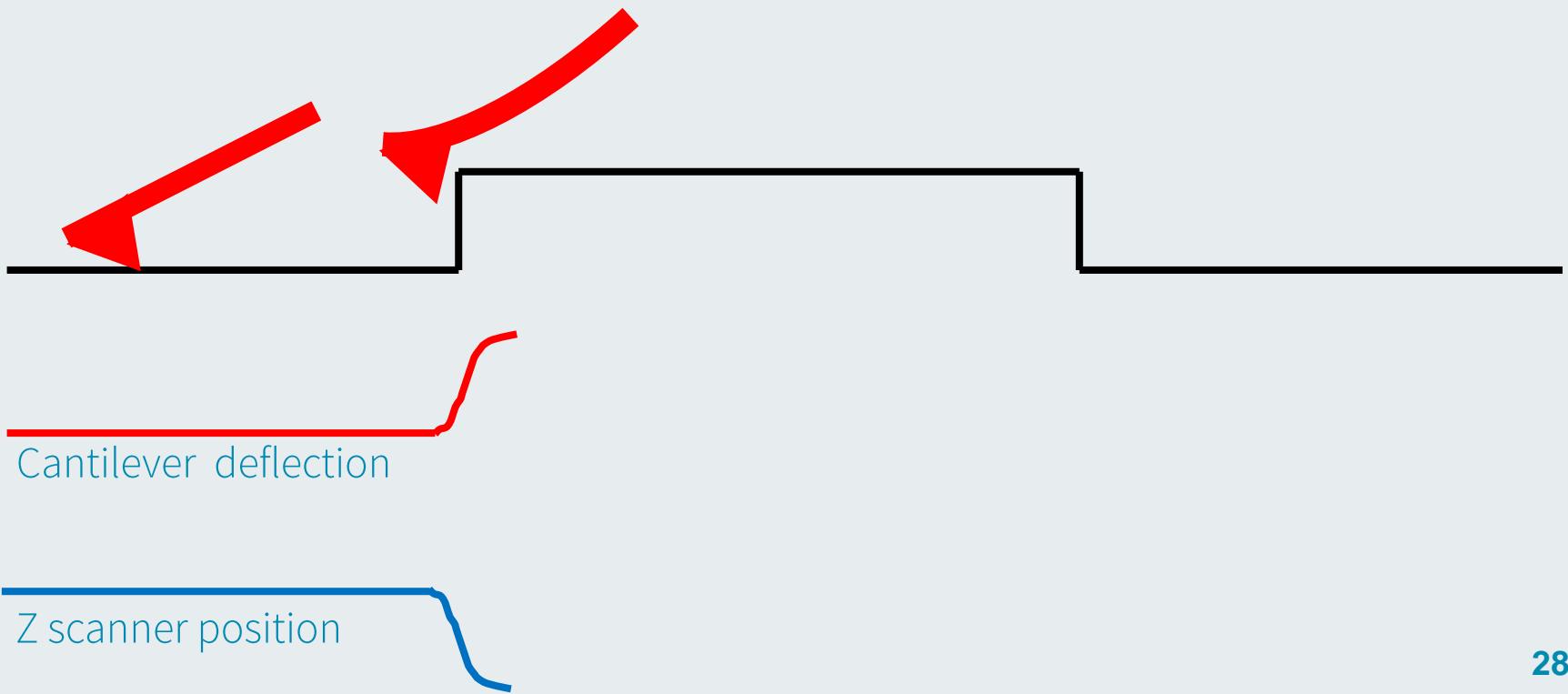
STATIC AFM: tip in permanent contact with the sample



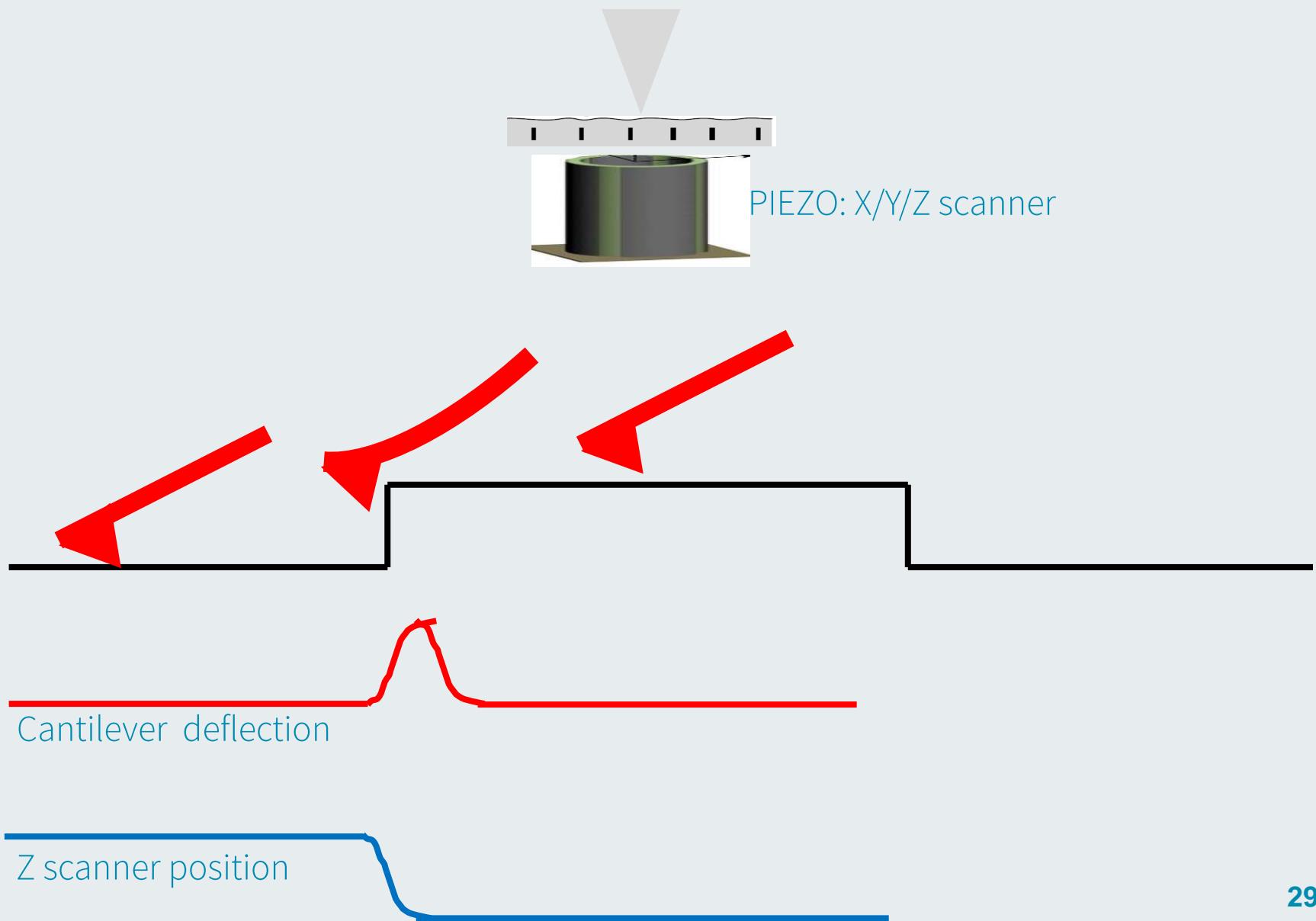
# Static AFM mode (contact mode) – The closed loop



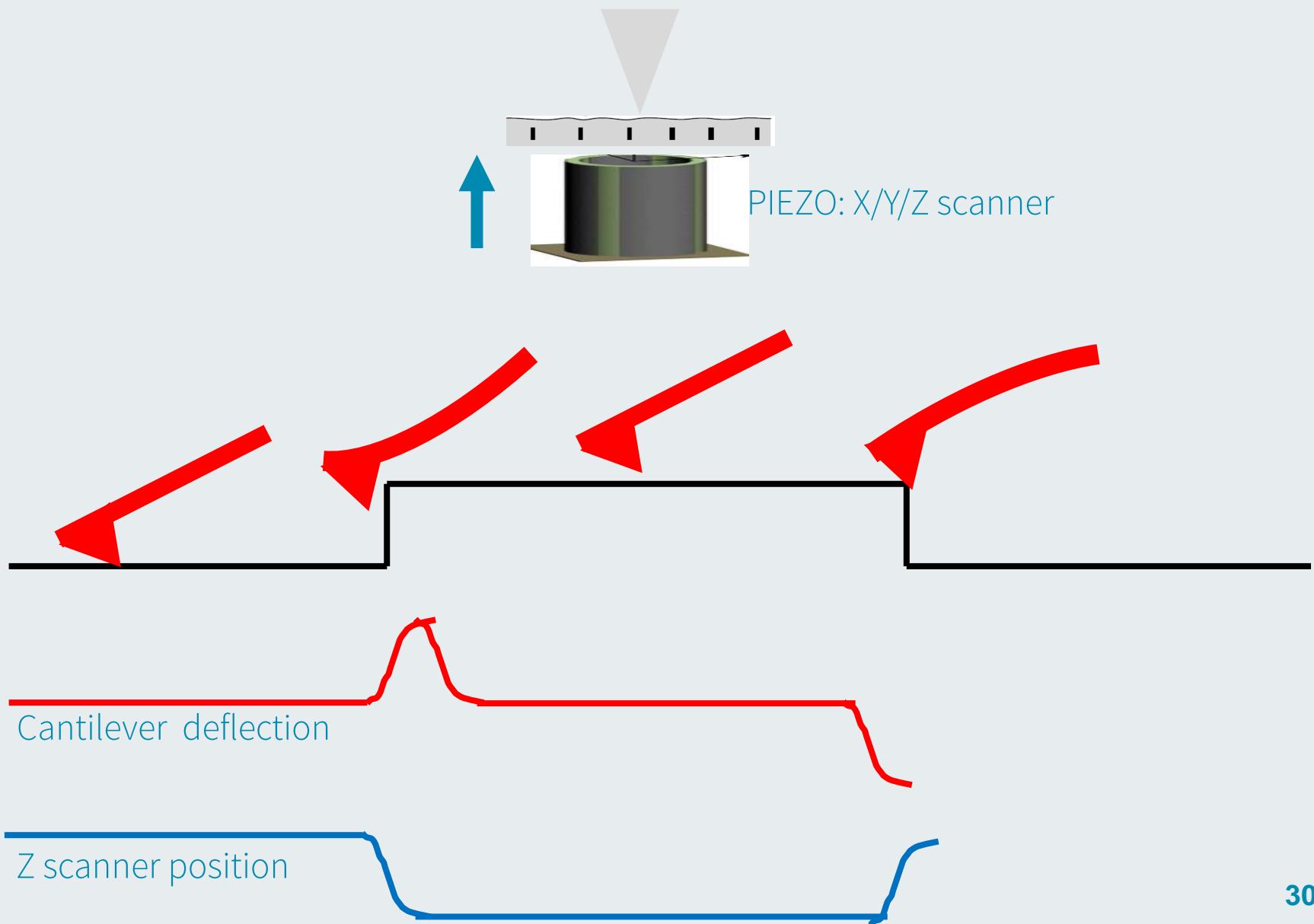
# Static AFM mode (contact mode) – The closed loop



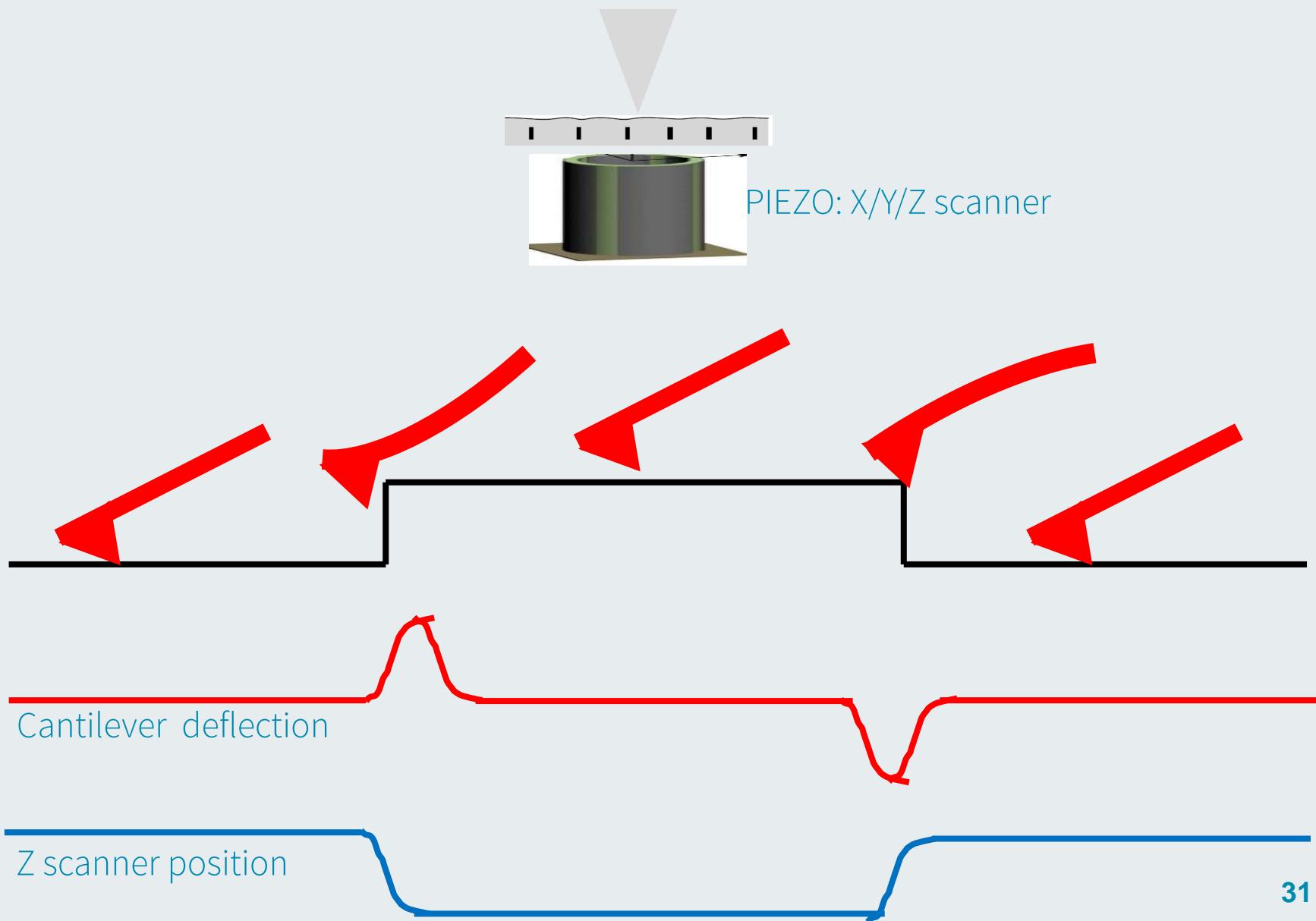
# Static AFM mode (contact mode) – The closed loop



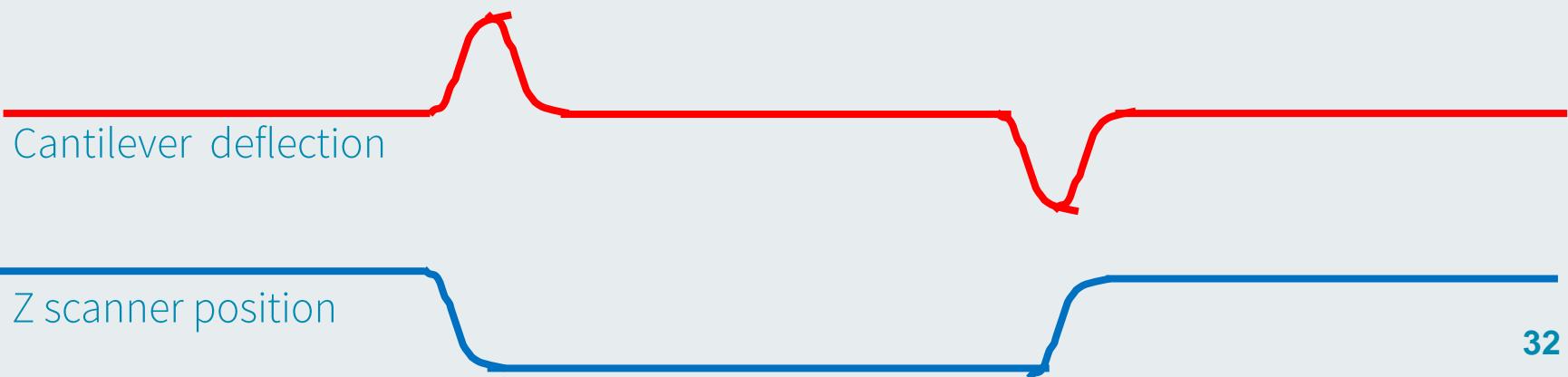
# Static AFM mode (contact mode) – The closed loop



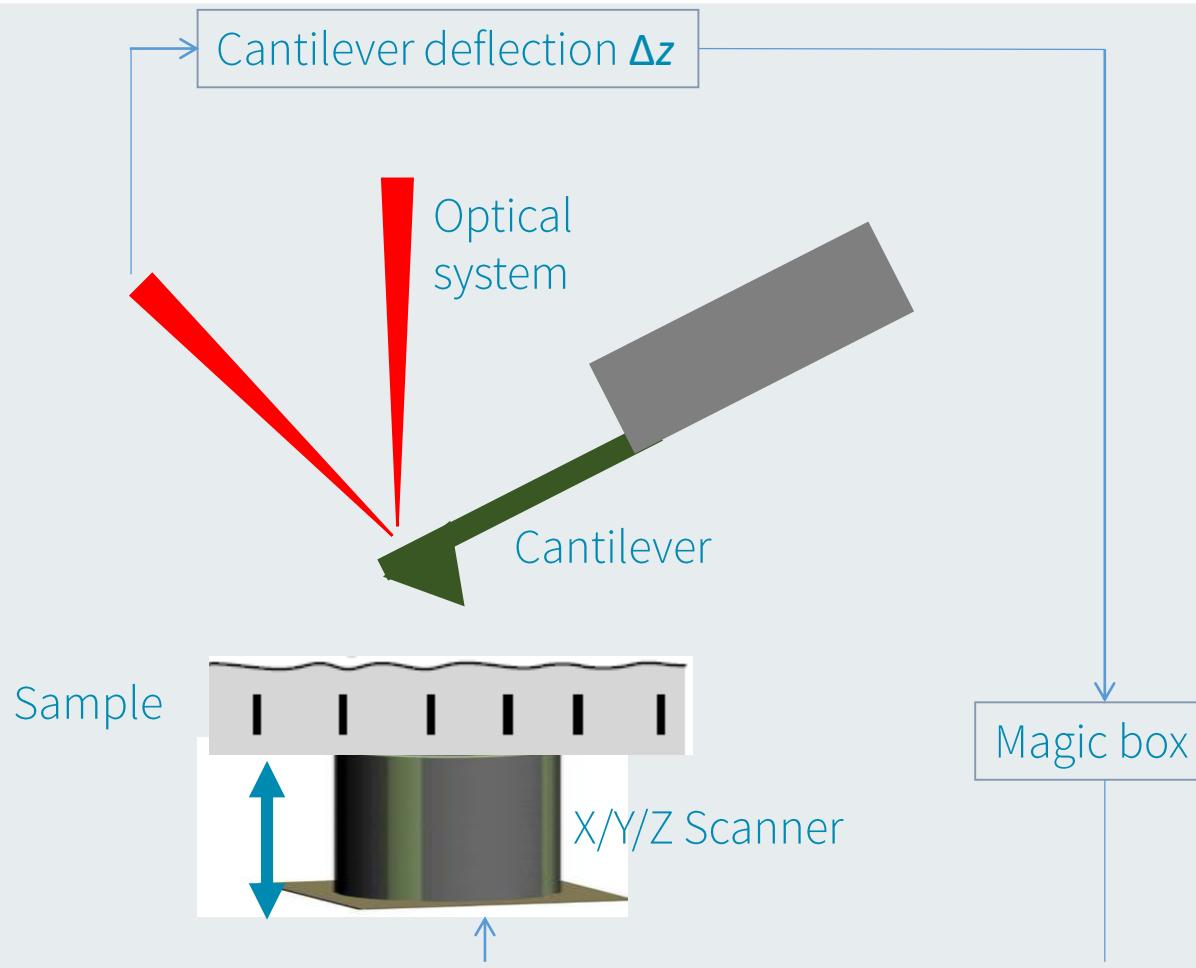
# Static AFM mode (contact mode) – The closed loop



# Constant deflection



# Static AFM mode (contact mode) – Operational scheme

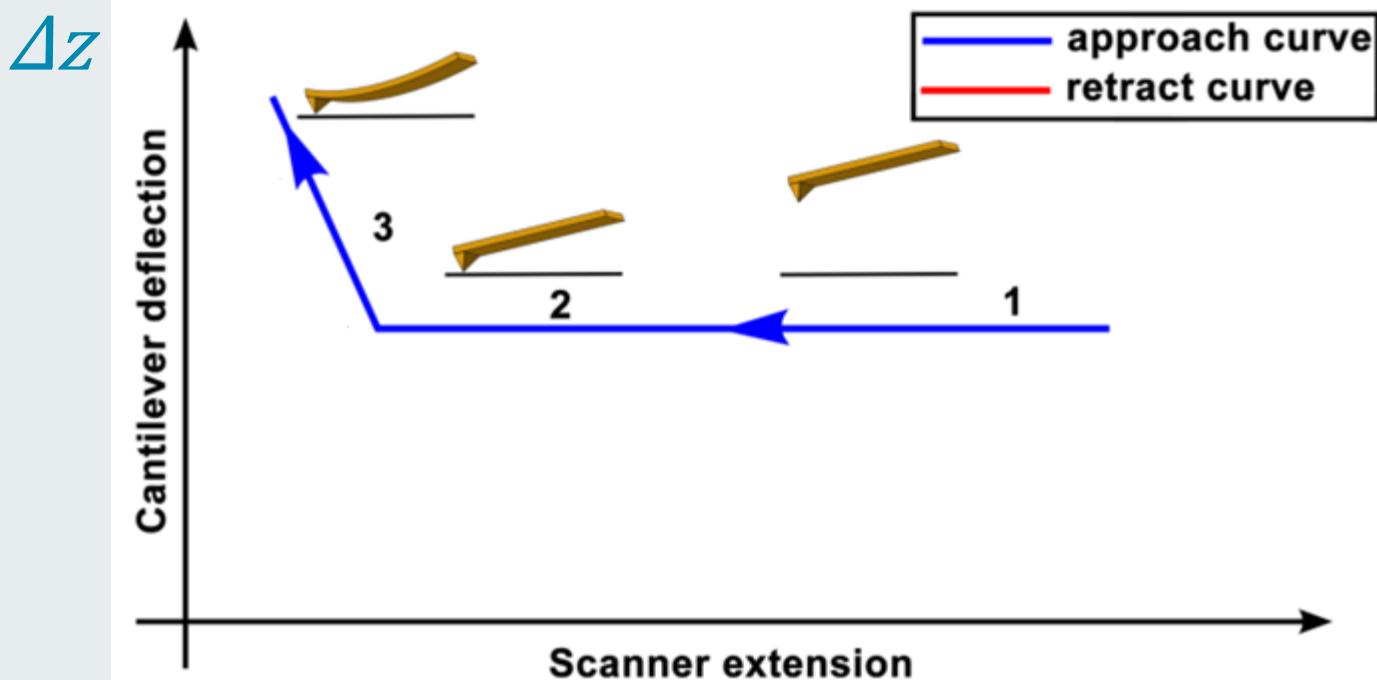


$$m\ddot{z} + \delta\dot{z} + kz = F_{interaction}(z) + F_0(\omega t)$$

$$\ddot{z} = 0, \dot{z} = 0, F_0(\omega t) = 0 \rightarrow F_{interaction}(z) = k\Delta z$$

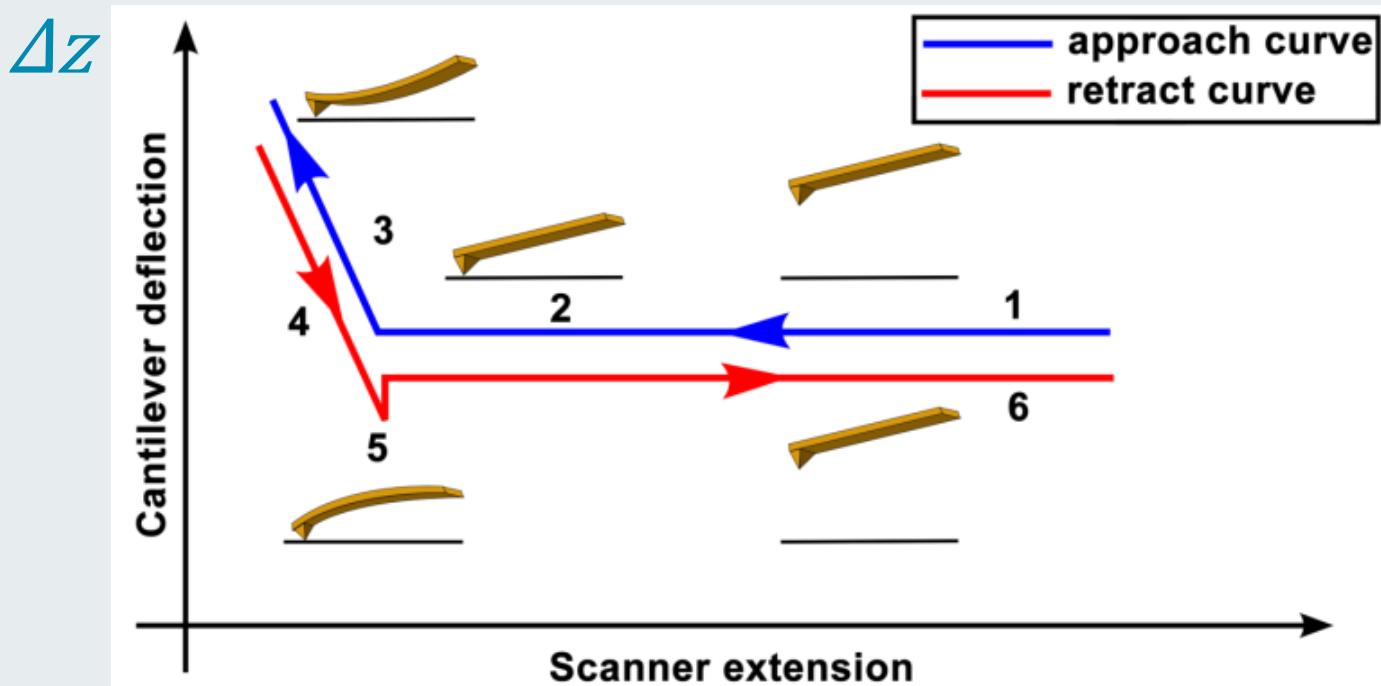
Hook Law  
33

# Static AFM mode (contact mode) – Force curves



Adapted from Polymer Science, Chapter 4, U. Maver et al., Intech, 2013

# Static AFM mode (contact mode) – Force curves



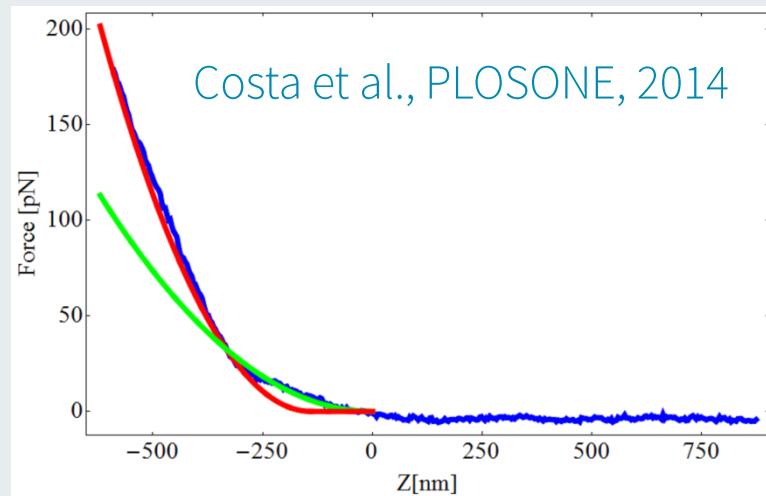
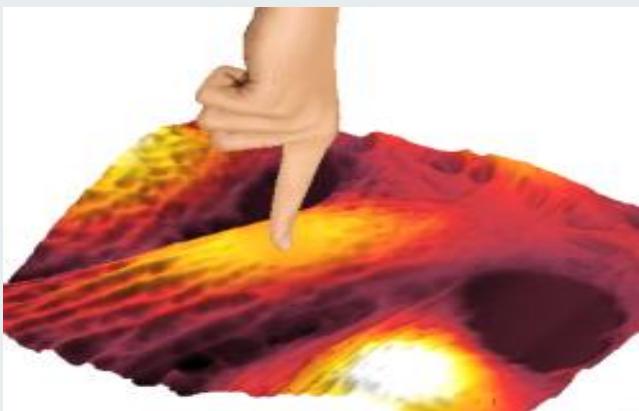
Adapted from Polymer Science, Chapter 4, U. Maver et al., Intech, 2013

H.-J. Butt, B. Cappella and M. Kappl,  
Surface Science Reports, 59, 1-152, 2005

# Static AFM mode (contact mode) – Force curves



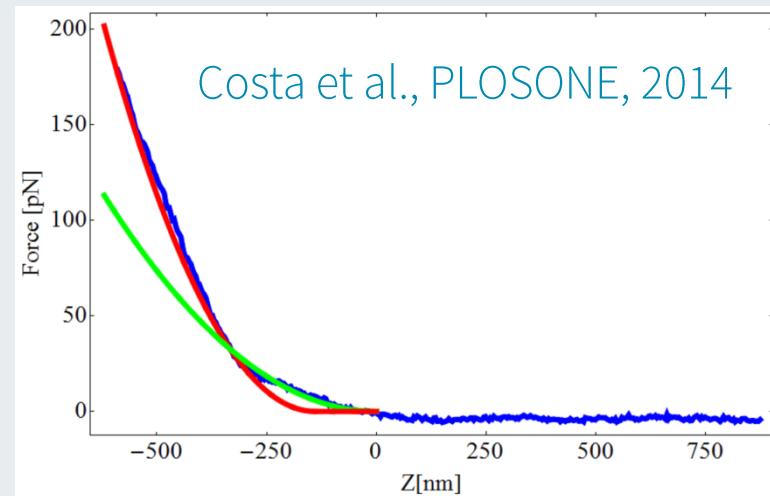
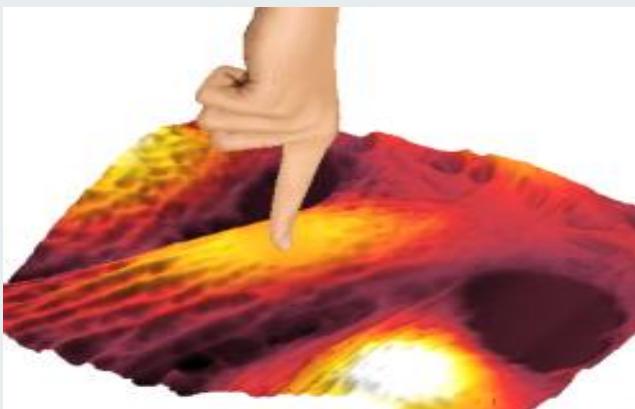
## Mechanics



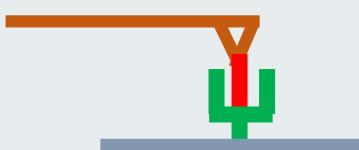
# Static AFM mode (contact mode) – Force curves



Mechanics



Molecular recognition



Ligand



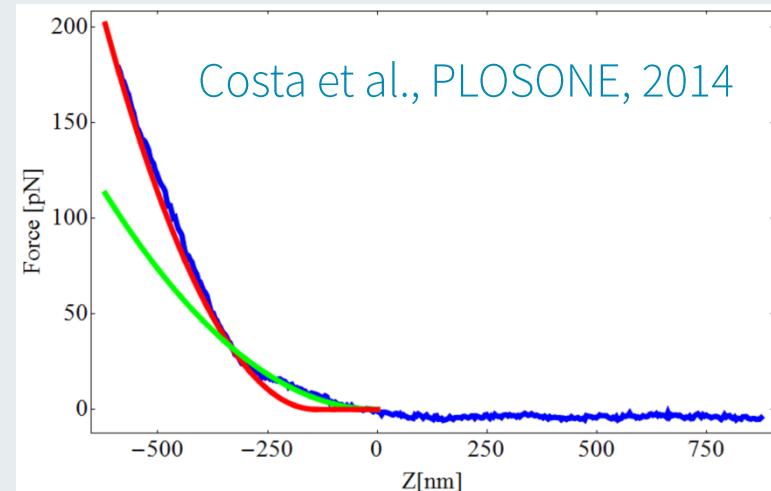
Receptor



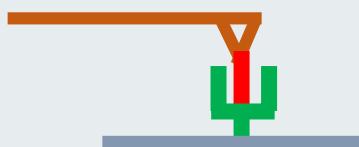
# Static AFM mode (contact mode) – Force curves



## Mechanics



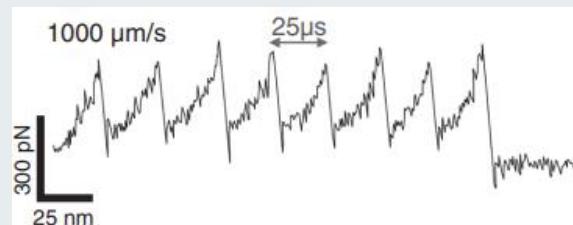
## Molecular recognition



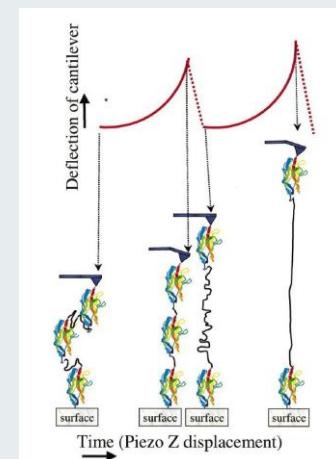
Ligand      Receptor



## Protein unfolding



F. Rico et al.  
Science,  
342(6159),  
741-743, 2013



Luigi  
Bubacco  
website

1) Introduction to Scanning Probe Microscopy

2) The Force



3) Methods

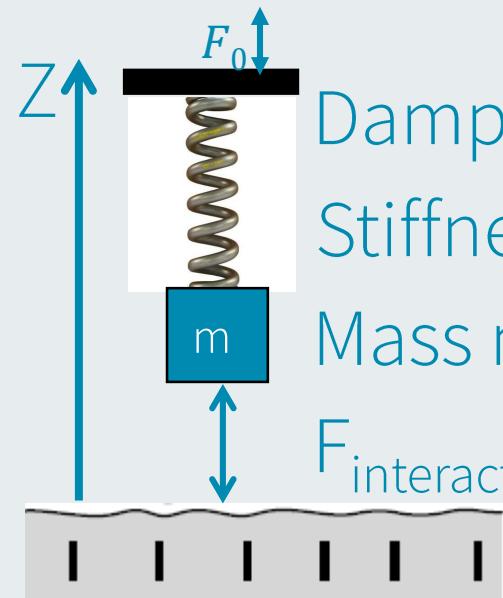
Cantilevers

Static and Dynamic AFM

4) Instruments

5) Advanced and novel AFM methods

$$m\ddot{z} + \delta\dot{z} + kz = F_{interaction}(z) + F_0(\omega t)$$



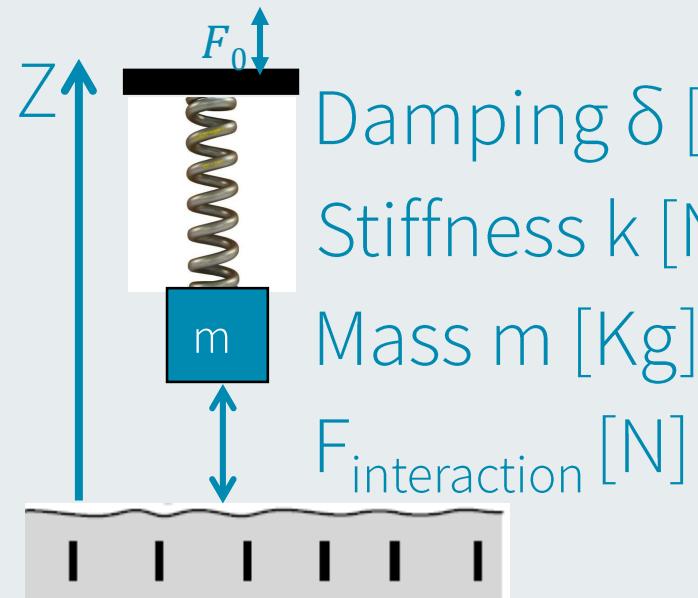
Damping  $\delta$  [N s /m]: environment, viscosity

Stiffness  $k$  [N/m]

Mass  $m$  [Kg]

$F_{interaction}$  [N]

$$m\ddot{z} + \delta\dot{z} + kz = F_{interaction}(z) + F_0(\omega t)$$



Damping  $\delta$  [N s /m]: environment, viscosity

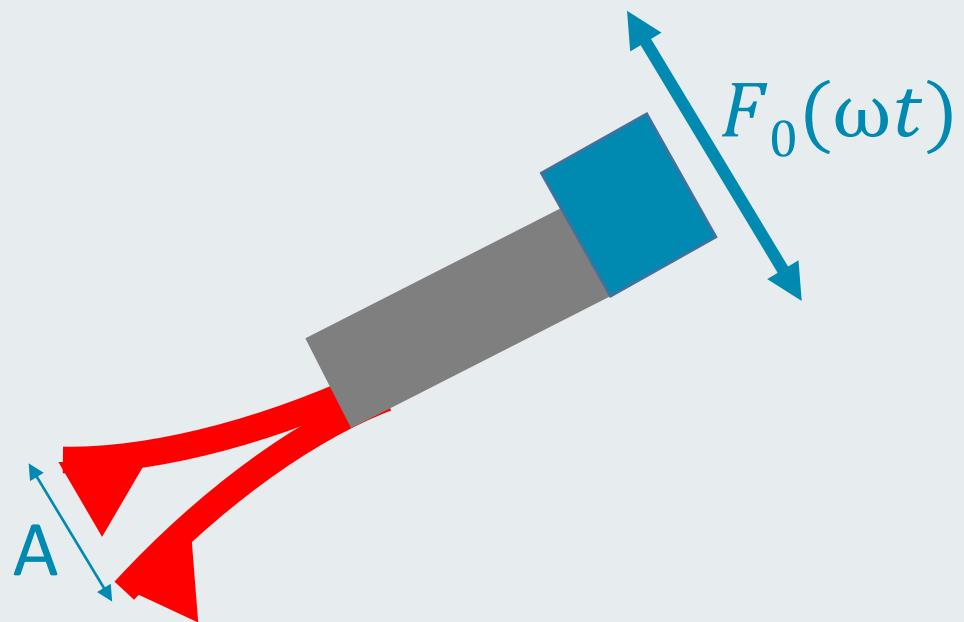
Stiffness  $k$  [N/m]

Mass  $m$  [Kg]

$F_{interaction}$  [N]

Resonance frequency

$$\omega_R = \sqrt{\frac{k}{m}}$$



$$m\ddot{z} + \delta\dot{z} + kz = F_{interaction}(z) + F_0(\omega t)$$

$F_{interaction}(z) = 0$  meaning no sample

*solution:*  $z = z_0 e^{i\omega t} = z_0 (\cos(\omega t) + i \sin(\omega t))$

$$z_0 = F_0 / (-m\omega^2 + i\delta\omega + k)$$

$$z_0 = F_0 / (-m\omega^2 + i\delta\omega + k)$$

$$z = a + ib$$

$$\text{Modulus: } |z| = \sqrt{a^2 + b^2}$$

$$\text{Phase: } \varphi = 2\arctan\left(\frac{b}{a+\sqrt{a^2+b^2}}\right)$$

# Dynamic AFM mode – Harmonic Oscillator



$$z_0 = F_0 / (-m\omega^2 + i\delta\omega + k)$$

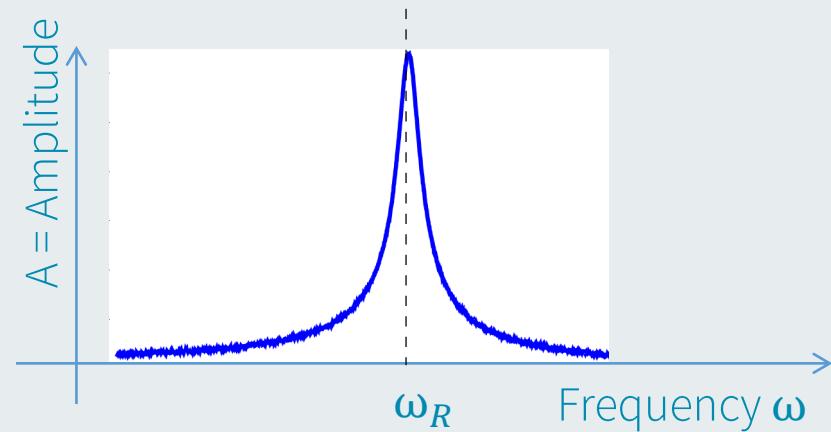
$$z = a + ib$$

$$\text{Modulus: } |z| = \sqrt{a^2 + b^2}$$

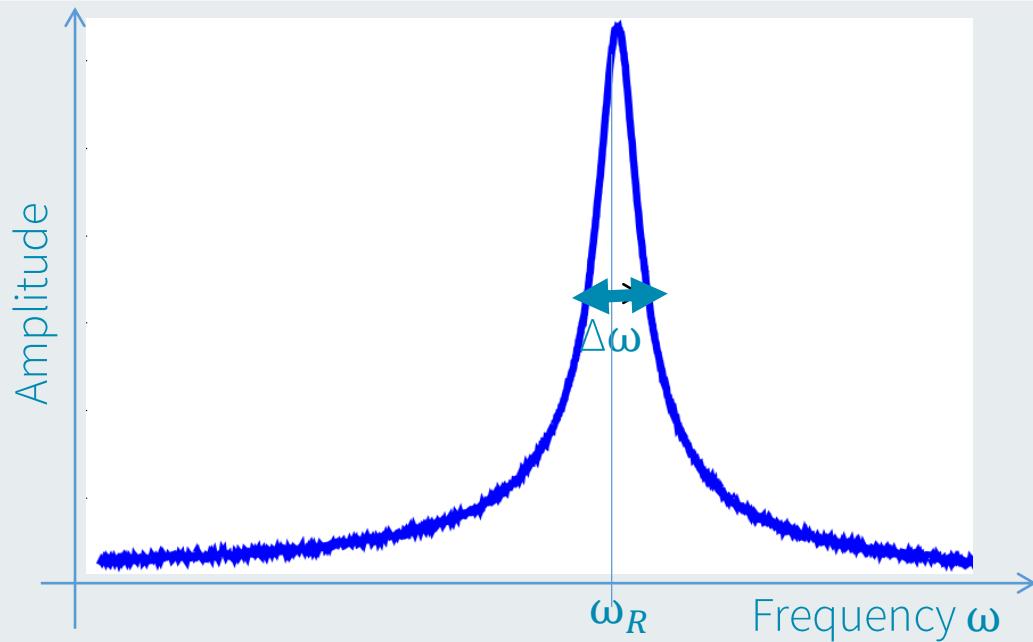
$$\text{Phase: } \varphi = 2\arctan\left(\frac{b}{a+\sqrt{a^2+b^2}}\right)$$

$$A = |z| = \frac{\frac{F_0}{m}}{\sqrt{(\omega_R^2 - \omega^2)^2 + \omega^2 \delta^2}}$$

$$\text{Phase} = \arctan(\varphi) = \frac{\delta\omega}{\omega_R^2 - \omega^2}$$



# Dynamic AFM mode – Harmonic Oscillator (Q factor)



Q factor

$$Q = \frac{\omega_R}{\Delta\omega}$$

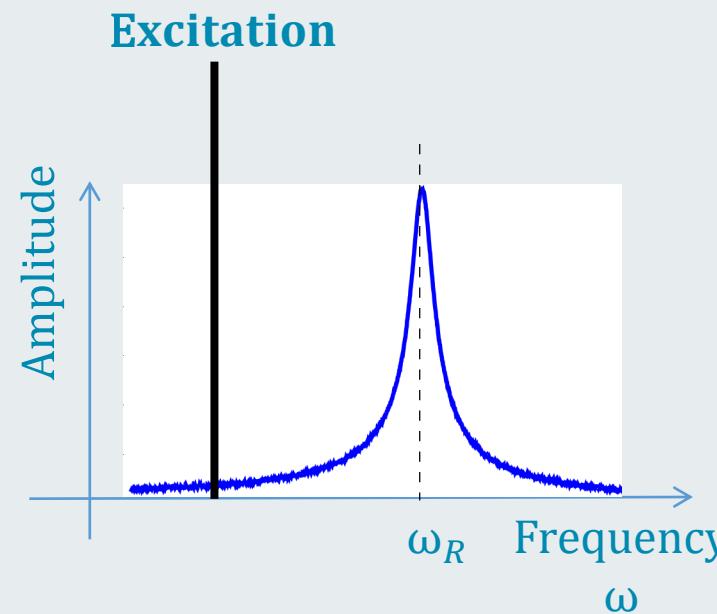
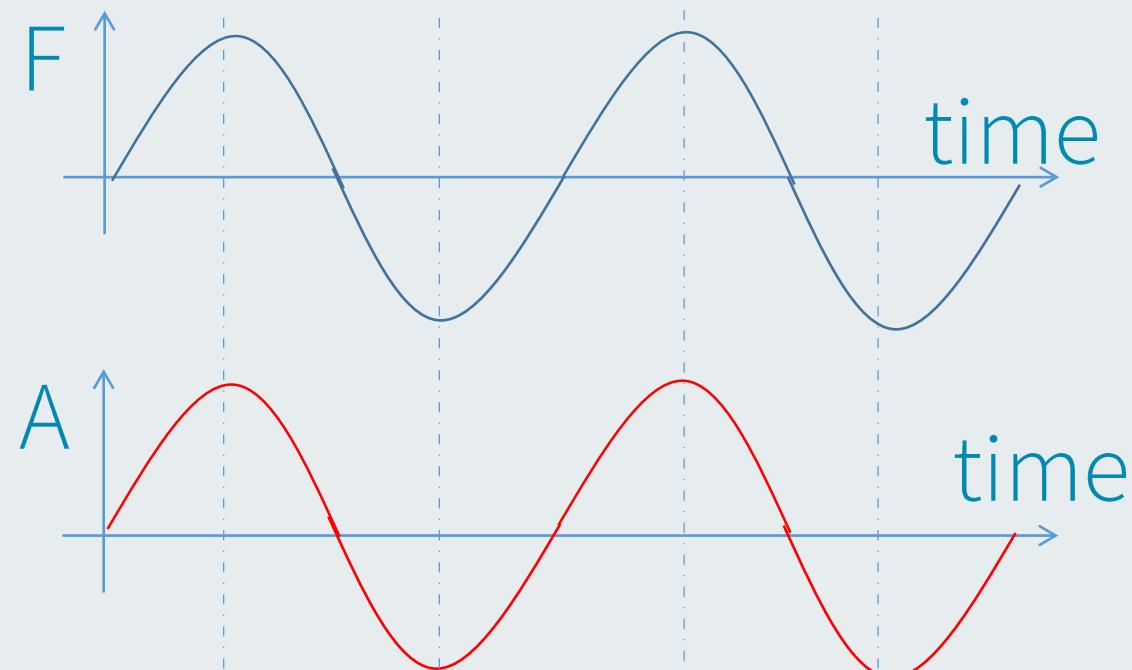
High Q



# Dynamic AFM mode – Harmonic Oscillator (phase)



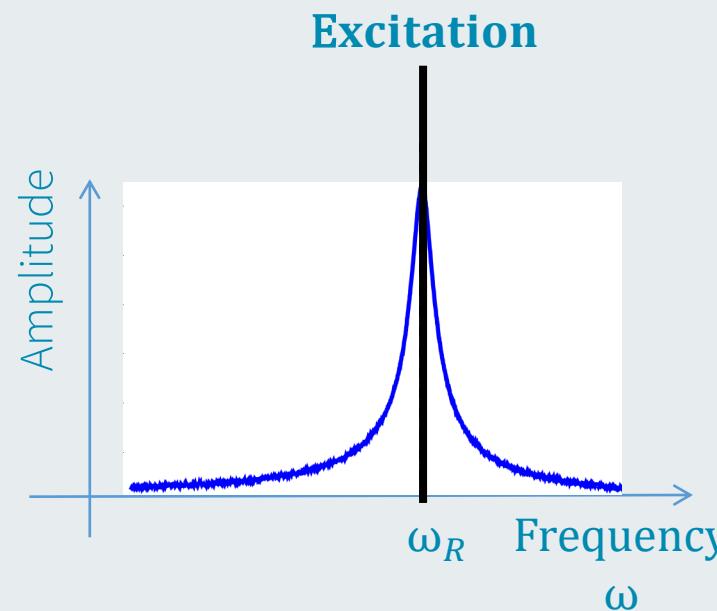
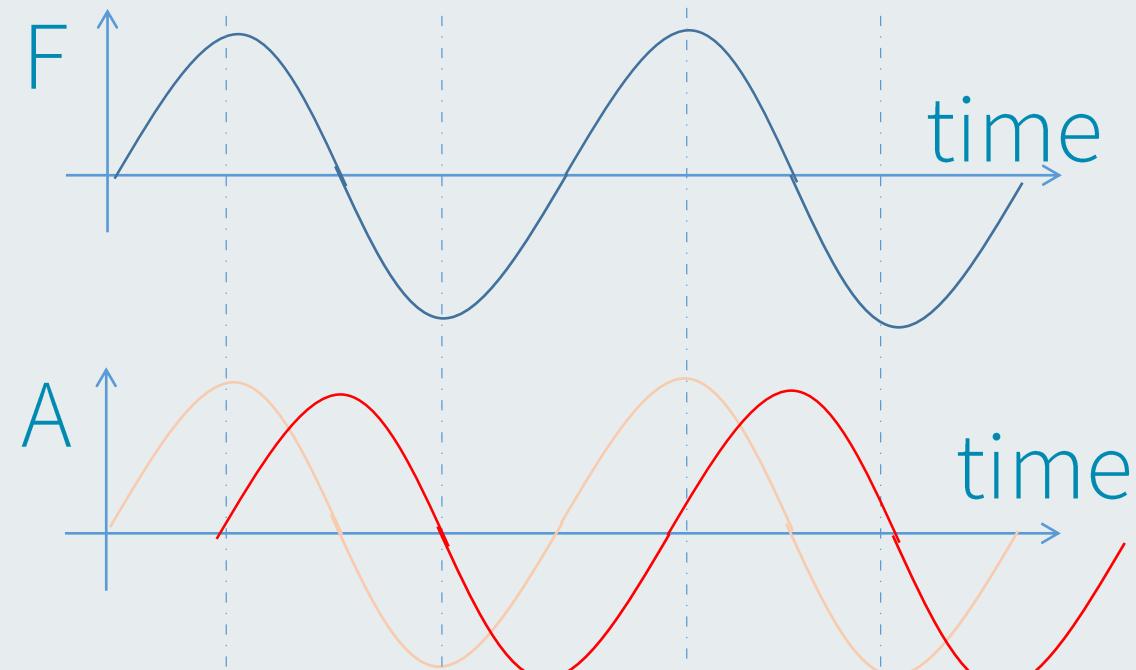
At low frequency



# Dynamic AFM mode – Harmonic Oscillator (phase)



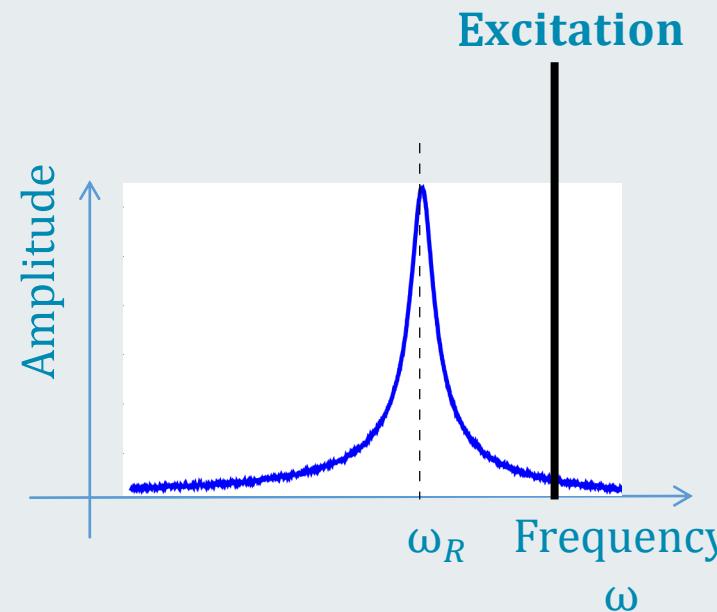
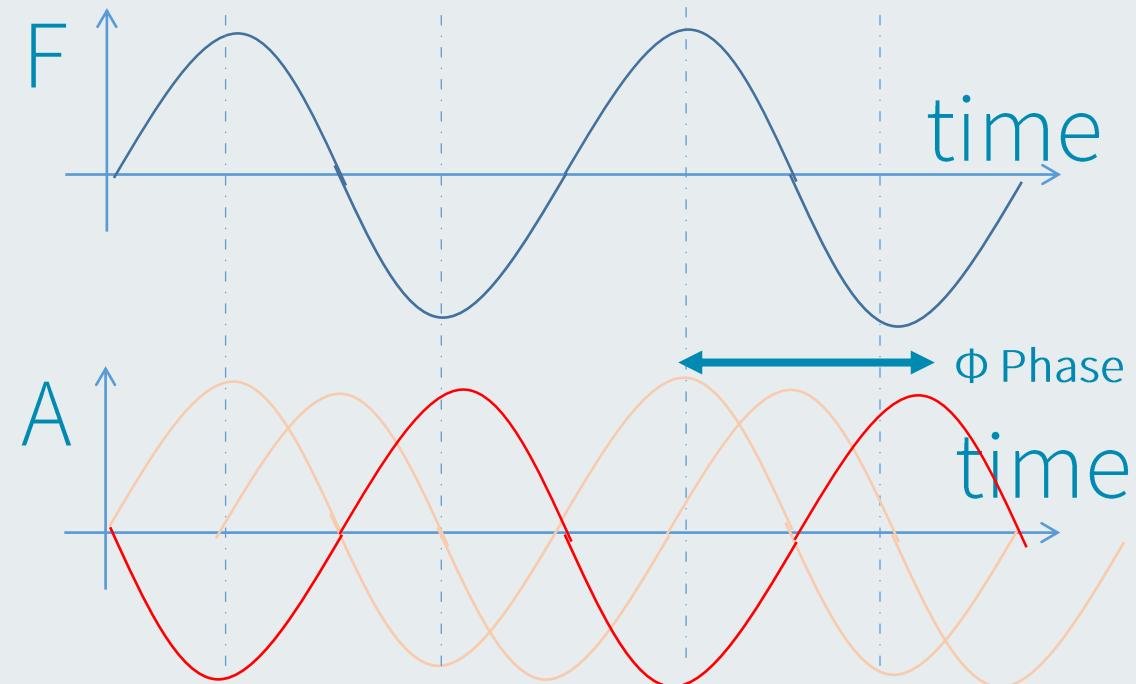
At resonance  $\omega_R$



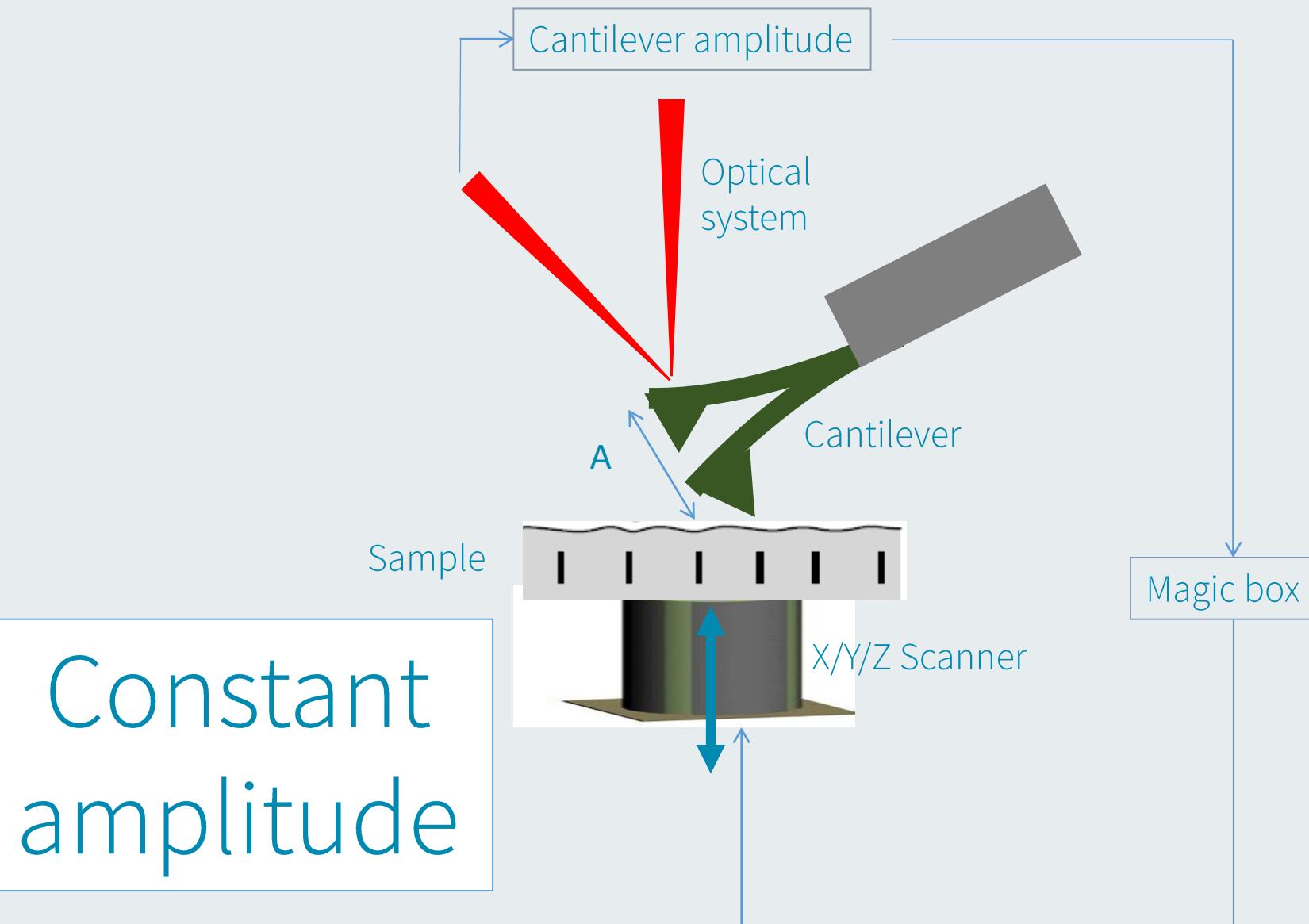
# Dynamic AFM mode – Harmonic Oscillator (phase)



After resonance



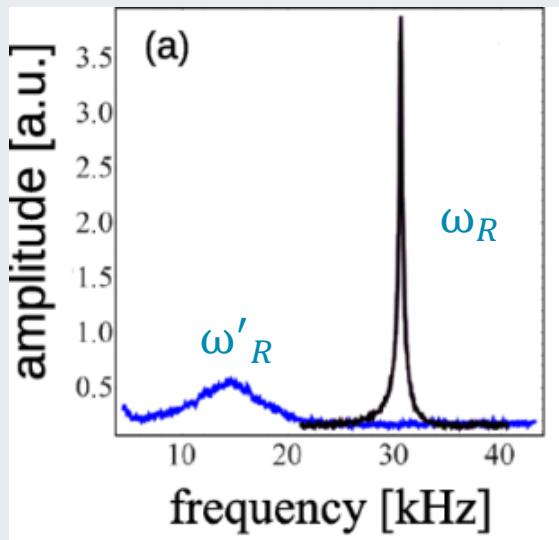
# Dynamic AFM mode (AM-AFM) – Operational scheme



# Dynamic AFM mode (AM-AFM) – in liquid, for biology



1) Part of the liquid participates (coupled) to cantilever motion

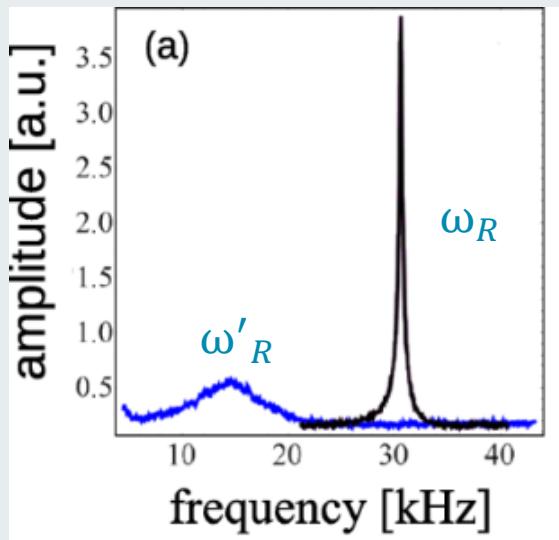


$$\omega_R = \sqrt{\frac{k}{m}} \rightarrow \omega'_R = \sqrt{\frac{k}{m + m_L}}$$

# Dynamic AFM mode (AM-AFM) – in liquid, for biology



1) Part of the liquid participates (coupled) to cantilever motion



$$\omega_R = \sqrt{\frac{k}{m}} \rightarrow \omega'_R = \sqrt{\frac{k}{m + m_L}}$$

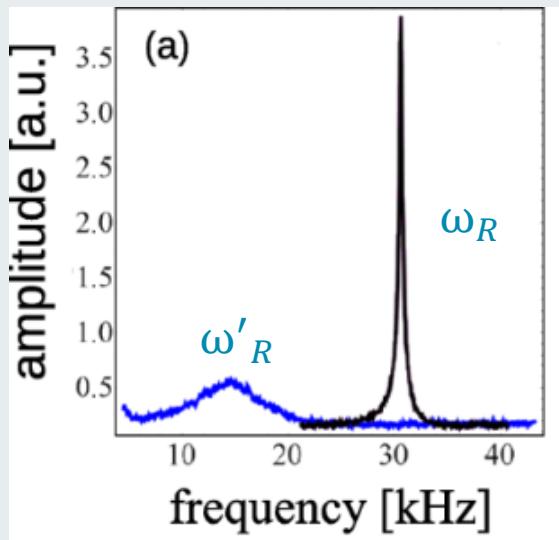
2) The resonance gets broader → decrease of Q factor. That's because water has higher viscosity than air  $\delta_{\text{liquid}} > \delta_{\text{air}}$

$$m\ddot{z} + \delta\dot{z} + kz = F_{\text{interaction}}(z) + F_0(\omega t)$$

# Dynamic AFM mode (AM-AFM) – in liquid, for biology



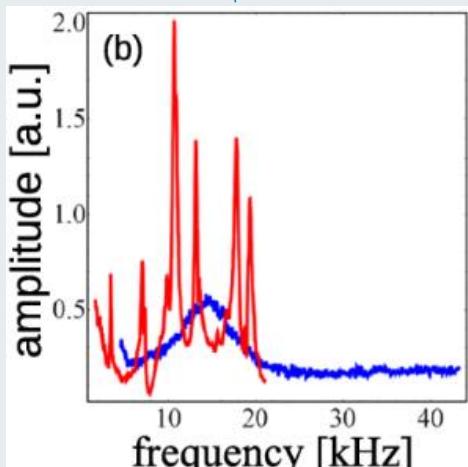
1) Part of the liquid participates (coupled) to cantilever motion



$$\omega_R = \sqrt{\frac{k}{m}} \rightarrow \omega'_R = \sqrt{\frac{k}{m + m_L}}$$

2) The resonance gets broader → decrease of Q factor. That's because water has higher viscosity than air  $\delta_{\text{liquid}} > \delta_{\text{air}}$

$$m\ddot{z} + \delta\dot{z} + kz = F_{\text{interaction}}(z) + F_0(\omega t)$$



3) When excited mechanically, the response of the tip is plenty of spurious peaks

1) Introduction to Scanning Probe Microscopy

2) The Force



3) Methods

Cantilevers

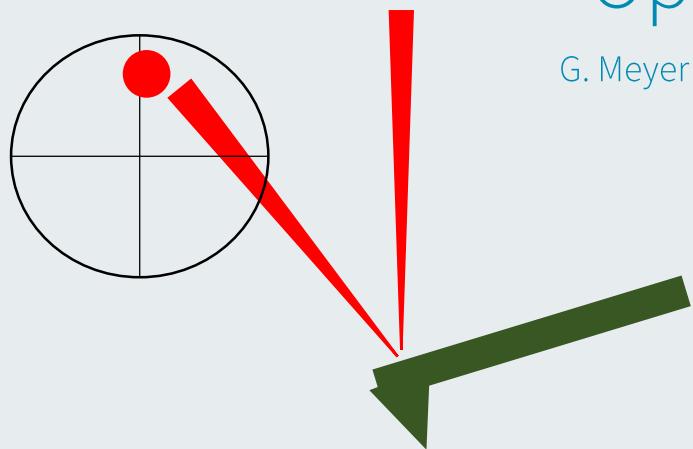
Static and Dynamic AFM

4) Instruments

5) Advanced and novel AFM methods

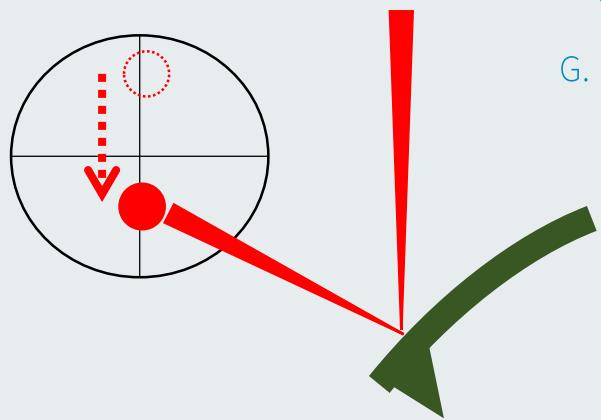
## Optical beam deflection

G. Meyer and N. M. Amer, Appl. Phys. Lett. 53, 1045 (1988).



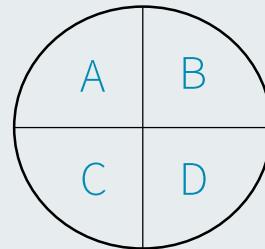
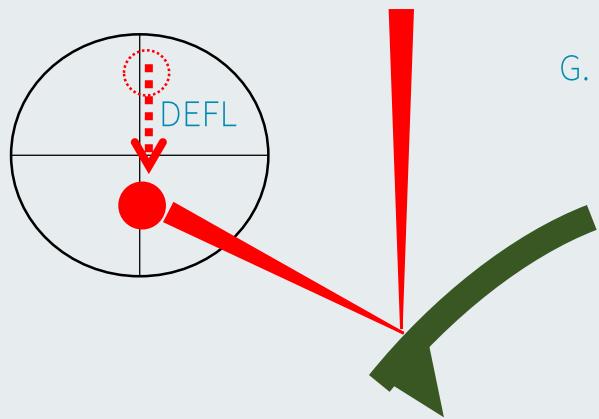
## Optical beam deflection

G. Meyer and N. M. Amer, Appl. Phys. Lett. 53, 1045 (1988).



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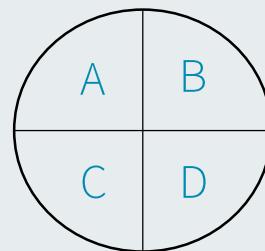
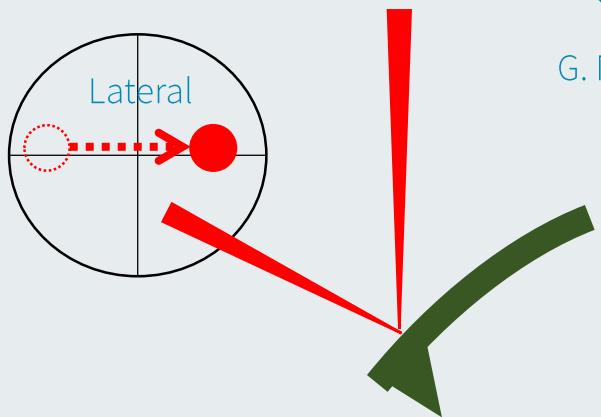


$$\text{DEFL} = \frac{(A+B)-(C+D)}{A+B+C+D}$$

$$\text{SUM} = A + B + C + D$$

## Optical beam deflection

G. Meyer and N. M. Amer, Appl. Phys. Lett. 53, 1045 (1988).



$$\text{DEFL} = \frac{(A+B)-(C+D)}{A+B+C+D}$$

$$\text{SUM} = A + B + C + D$$

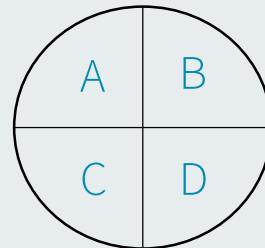
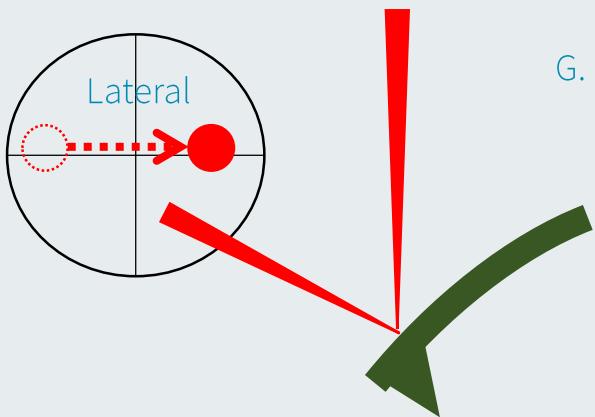
$$\text{Lateral} = \frac{(A+C)-(B+D)}{A+B+C+D}$$

# Tip position measurement



## Optical beam deflection

G. Meyer and N. M. Amer, Appl. Phys. Lett. 53, 1045 (1988).



$$\text{DEFL} = \frac{(A+B)-(C+D)}{A+B+C+D}$$

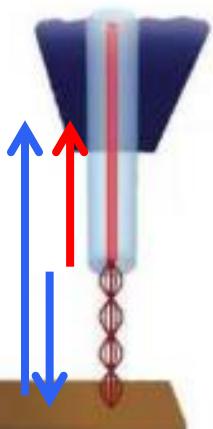
$$\text{SUM} = A + B + C + D$$

$$\text{Lateral} = \frac{(A+C)-(B+D)}{A+B+C+D}$$

## Interferometry

D. Rugar, H. J. Mamin, R. Erlandsson, J. E. Stern, and B. D. Terris, Rev. Sci. Instrum. 59, 2337 (1988).

Drawback:  
DRIFT!!!



Interference of red and blue beams

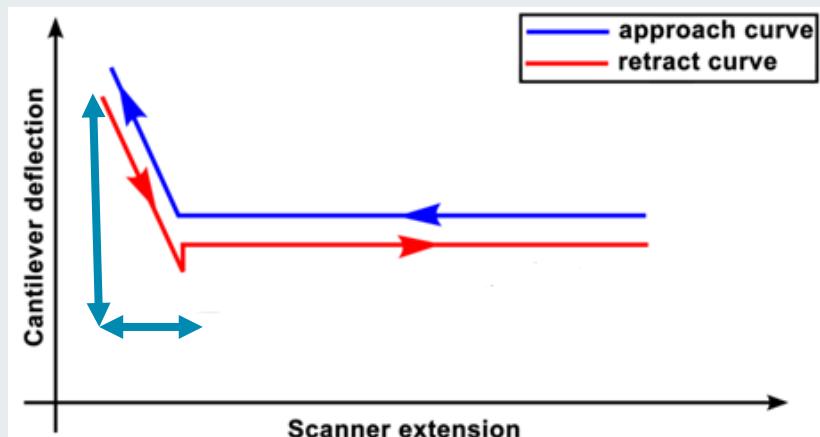
$$\xrightarrow{\quad\quad\quad} I(d)$$

$$I(d) = I_0 + \Delta I_0 \sin \left( \frac{4\pi}{\lambda} d + \phi \right)$$

B. Hogenboom Imp. College London

## -1- Detector sensitivity

Acquire a force curve on a very rigid surface (i.e. mica or silicon)



Condition:

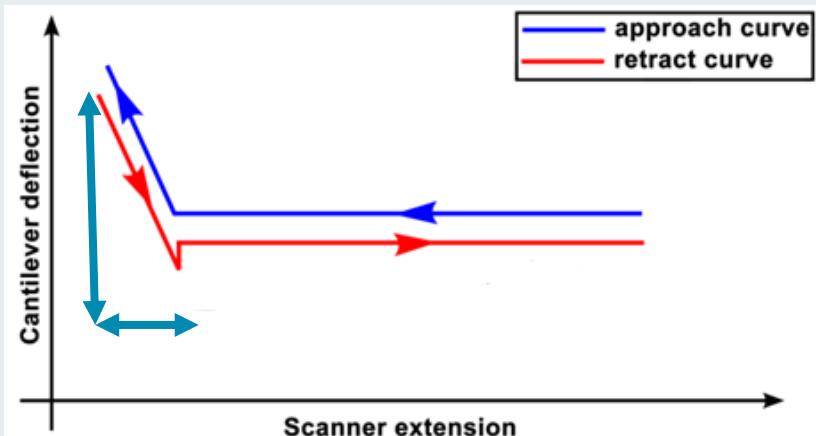
scanner extension (nm) = cantilever deflection (nm)

scanner extension (nm) =  $\Phi \times$  cantilever deflection (V)

$$\Phi = \frac{\text{scanner extension}}{\text{cantilever deflection}} \quad [\text{nm/V}]$$

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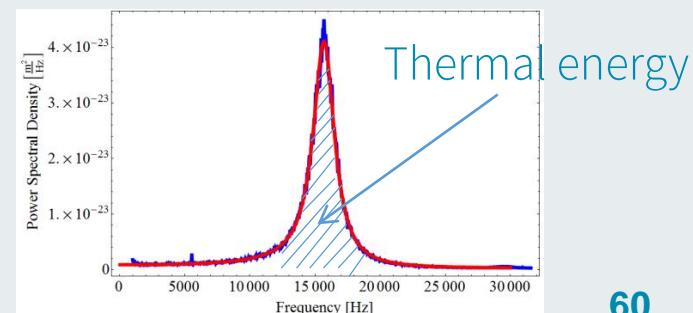
$$\Phi = \frac{\text{scanner extension}}{\text{cantilever deflection}} \quad [\text{nm/V}]$$

## -2- Cantilever stiffness

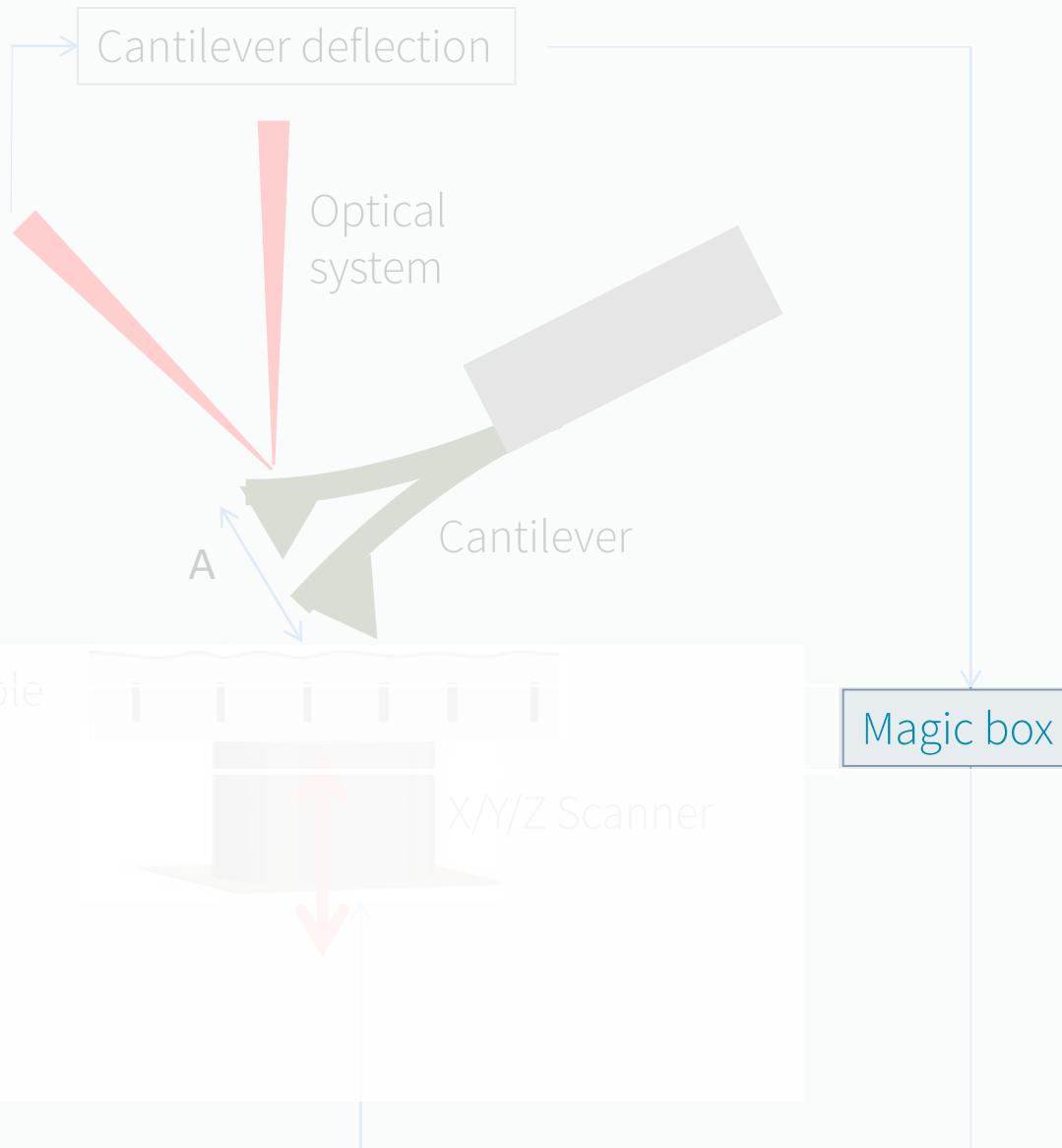
Thermal method

Thermal energy =  $\frac{1}{2} K_B T$  = Cantilever energy =  $\frac{1}{2} k \text{ deflection}^2$

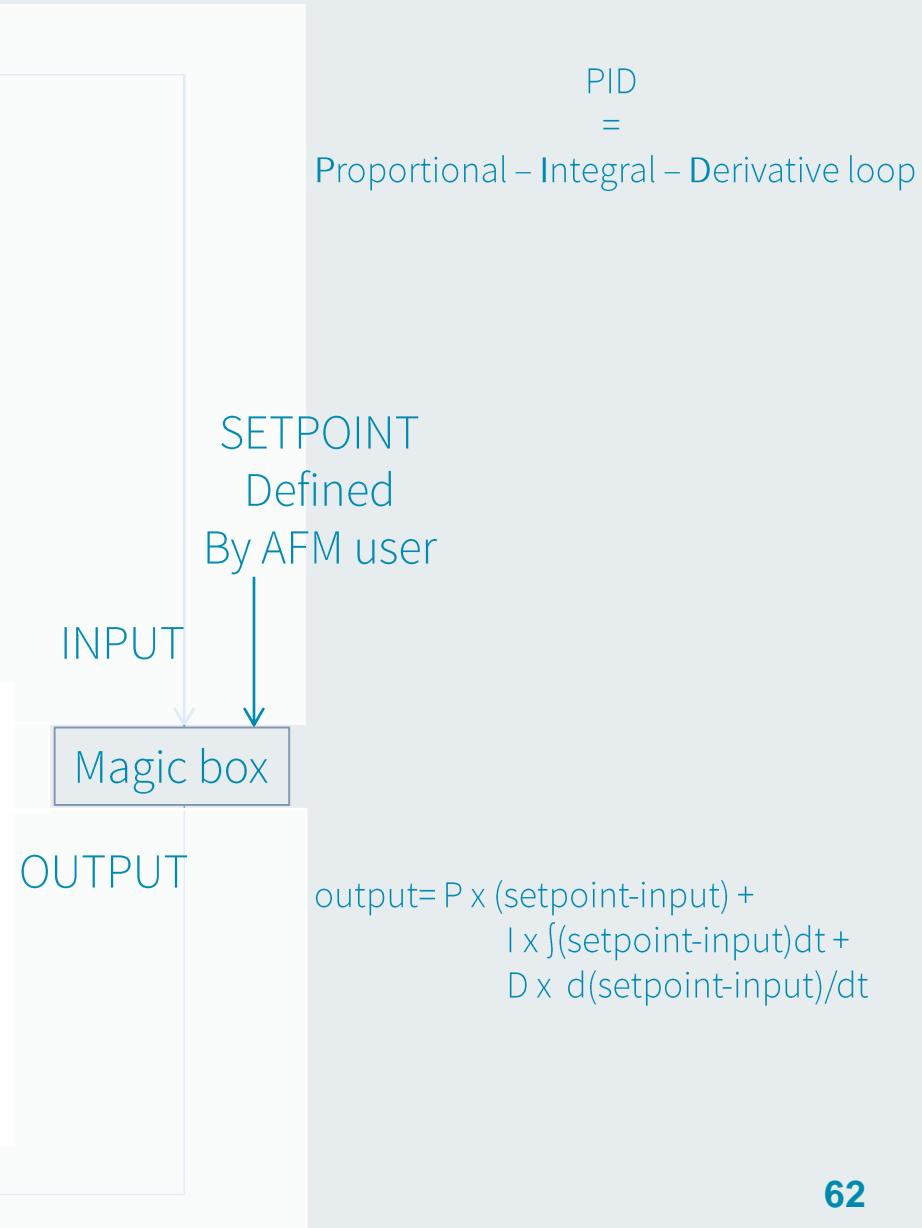
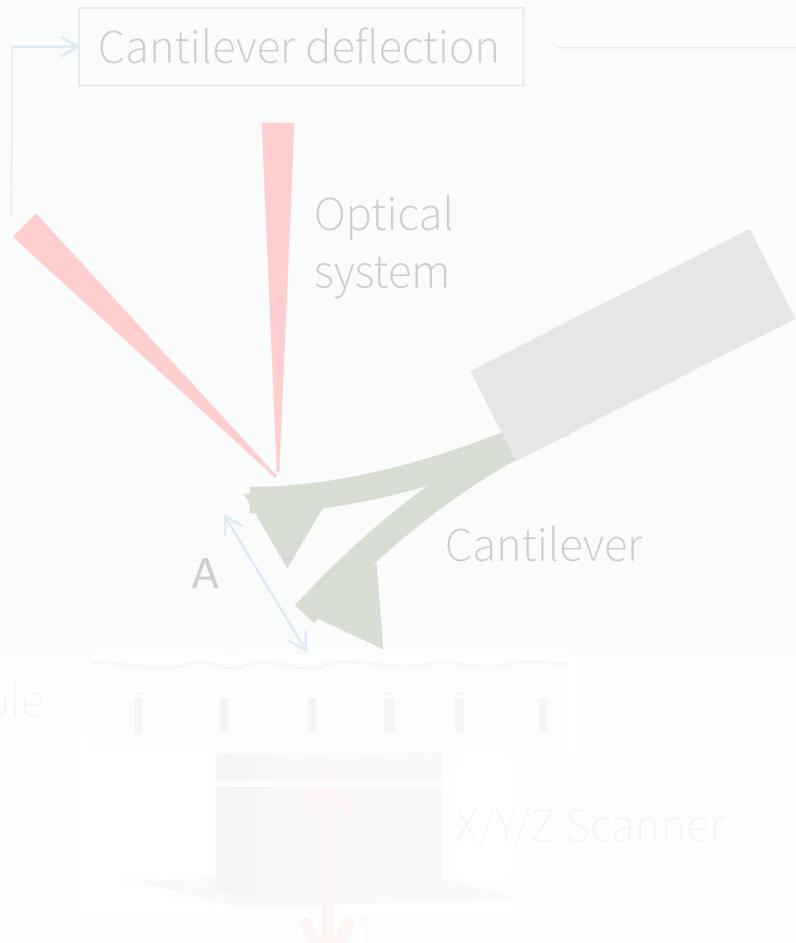
$$k = \frac{K_B T}{\text{deflection}^2(\omega)} \quad [\text{N/m}]$$



# The « magic box »



# The « magic box »



# Tip excitation

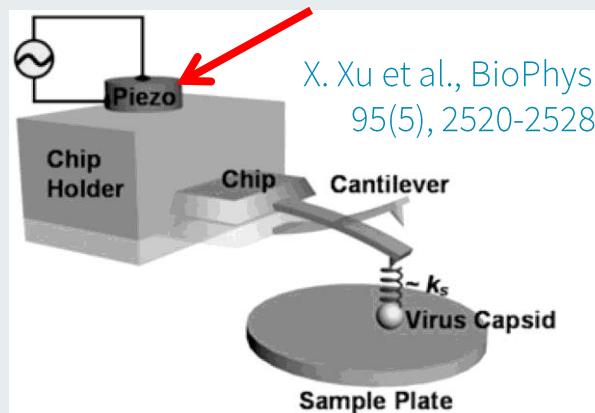


## -1- Piezo-dither mode

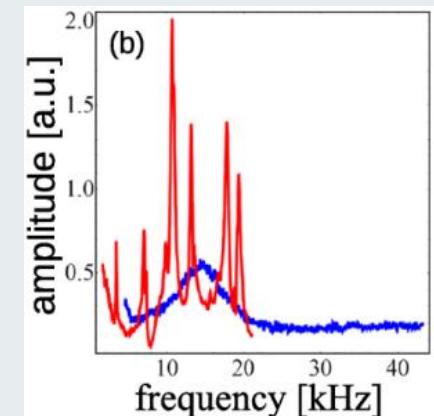
Present in all AFMs

Drawback:

Excitation in liquid



X. Xu et al., BioPhys. Journal, 95(5), 2520-2528, 2008



# Tip excitation

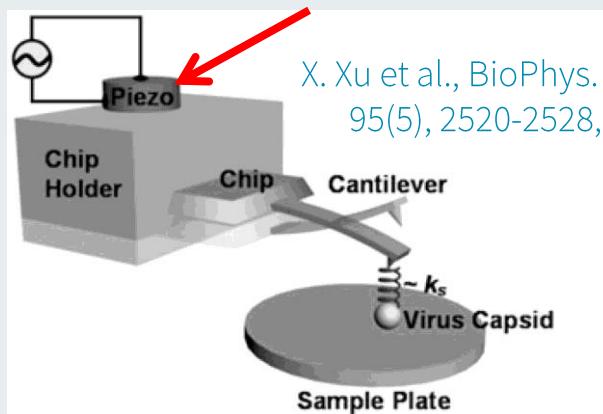


## -1- Piezo-dither mode

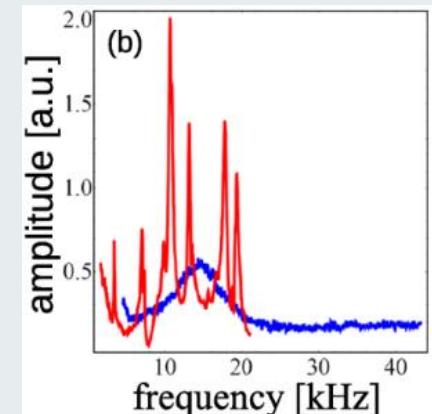
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Drawback:

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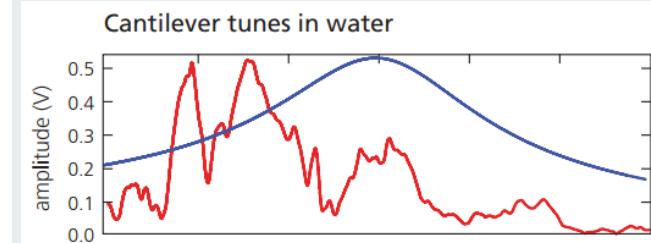
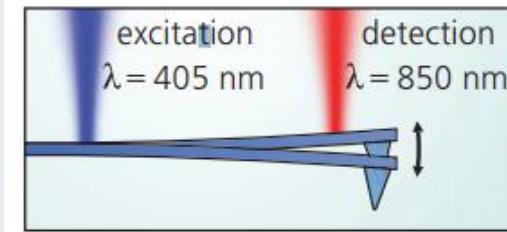
X. Xu et al., BioPhys. Journal, 95(5), 2520-2528, 2008



## -2- Photothermal excitation

Provided by Asylum Research

Makes use of a 2<sup>nd</sup> laser (blue) to excite the cantilever base



From Asylum Research website

# Tip excitation

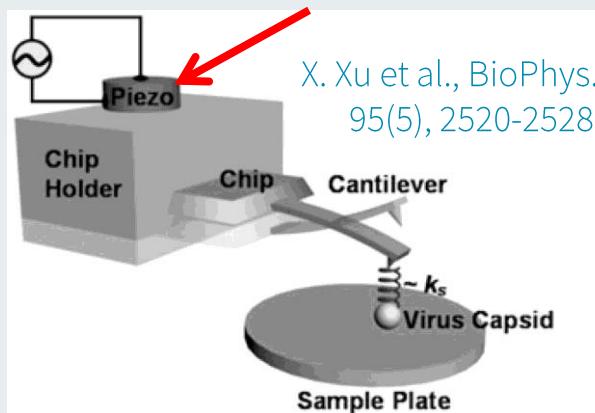


## -1- Piezo-dither mode

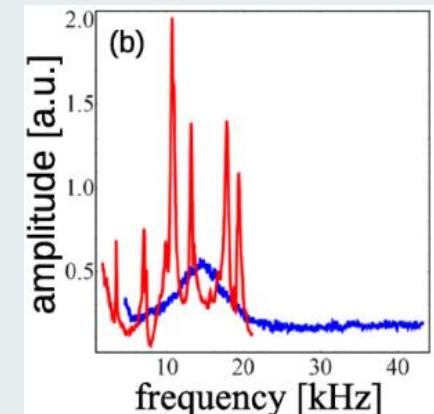
Present in all AFMs

Drawback:

Excitation in liquid



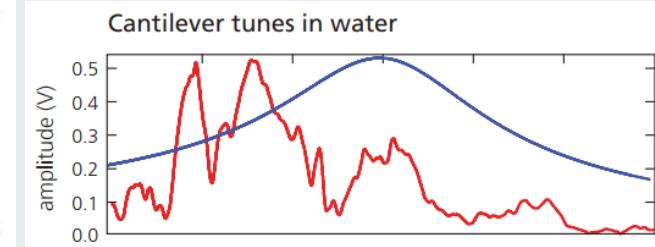
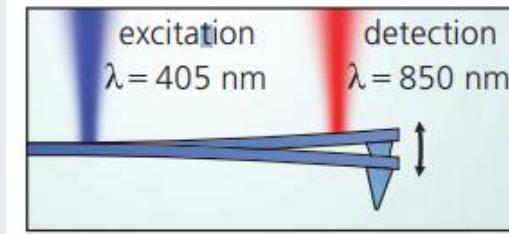
X. Xu et al., BioPhys. Journal, 95(5), 2520-2528, 2008



## -2- Photothermal excitation

Provided by Asylum Research

Makes use of a 2<sup>nd</sup> laser (blue) to excite the cantilever base



From Asylum Research website

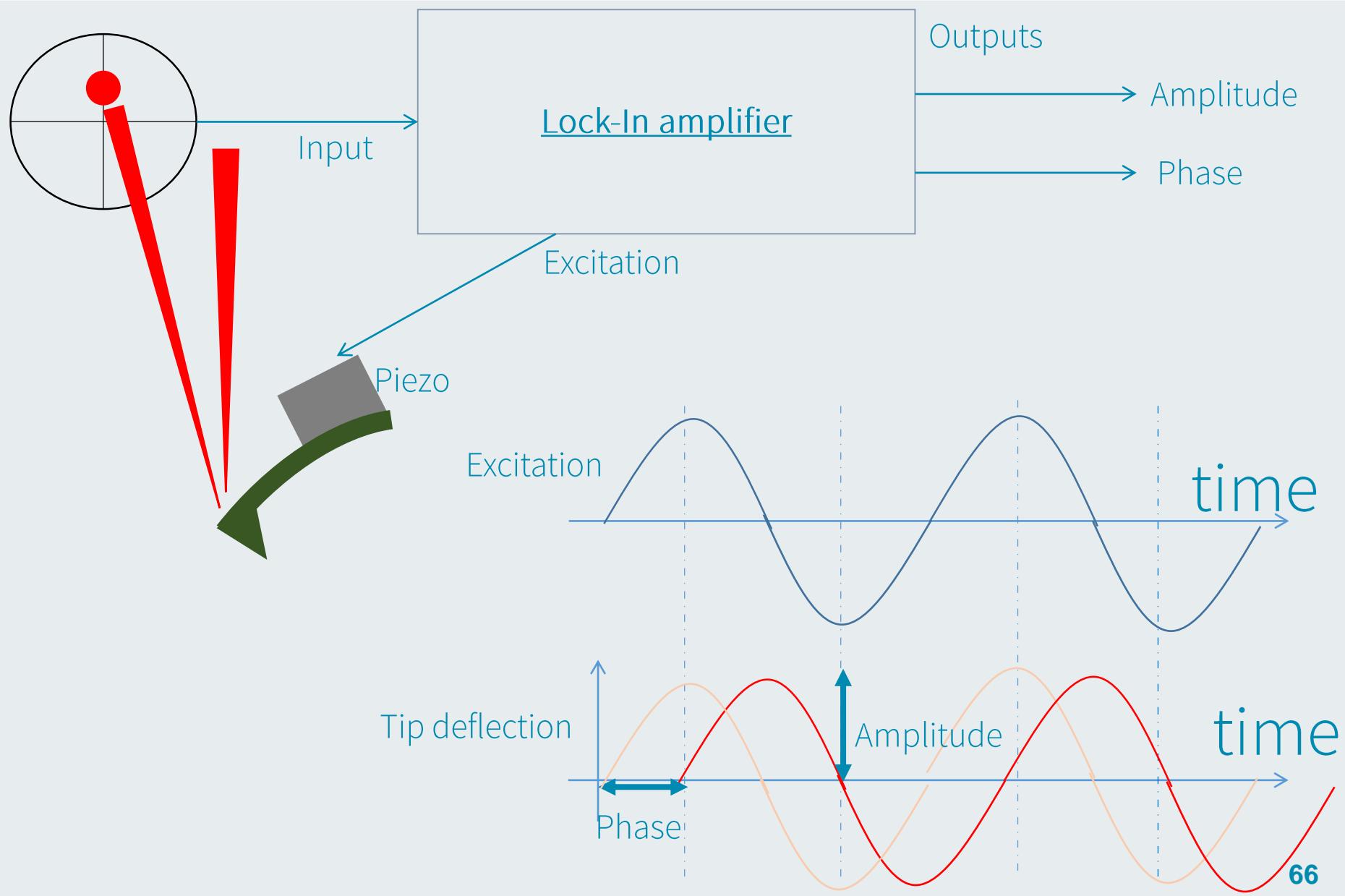
## -3- Magnetic excitation

Provided by AGILENT

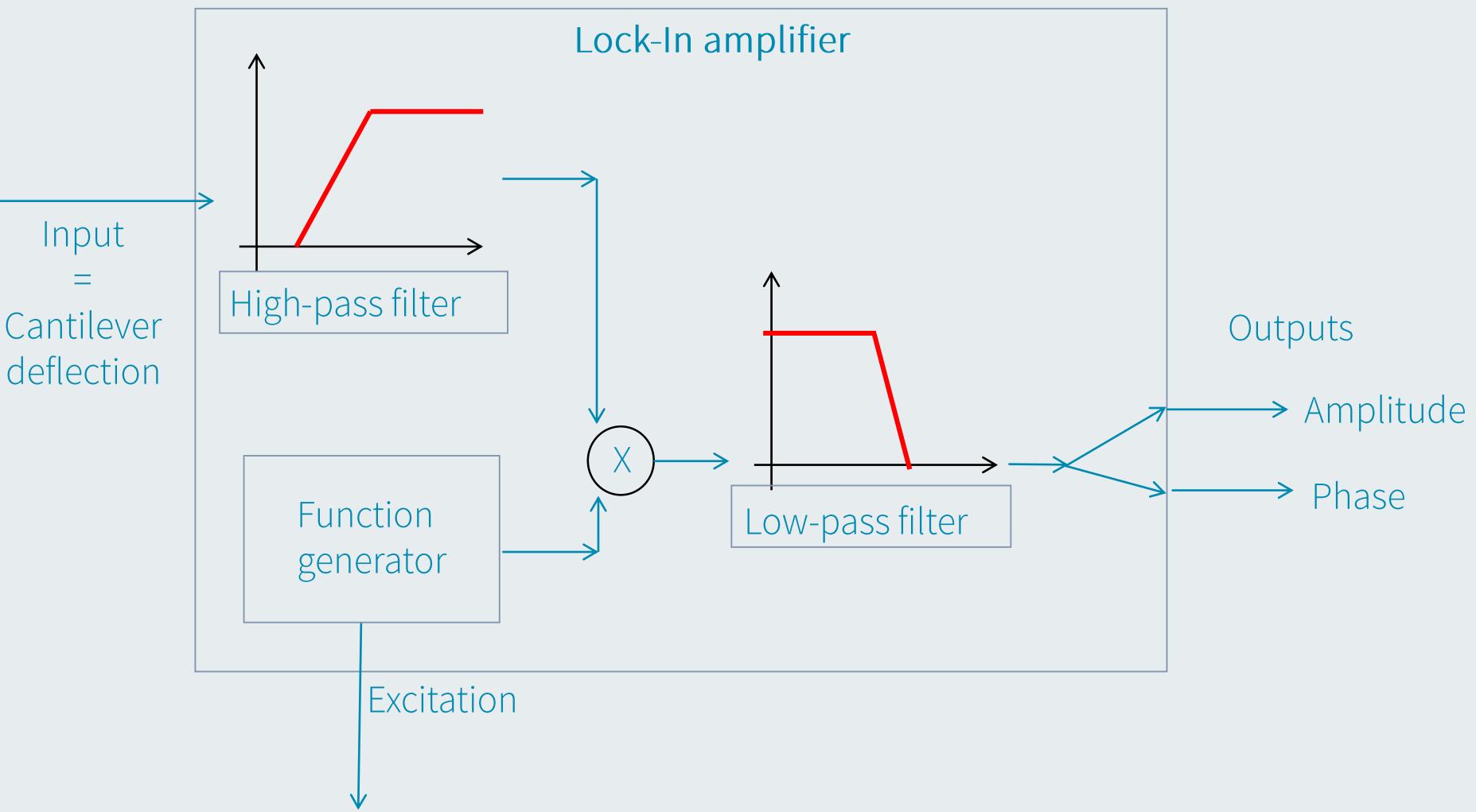
Makes use of a magnetic tip

Cantilever stiffness limitations

# Lock-in Amplifier



# Lock-in Amplifier



1) Introduction to Scanning Probe Microscopy

2) The Force



3) Methods

Cantilevers

Static and Dynamic AFM

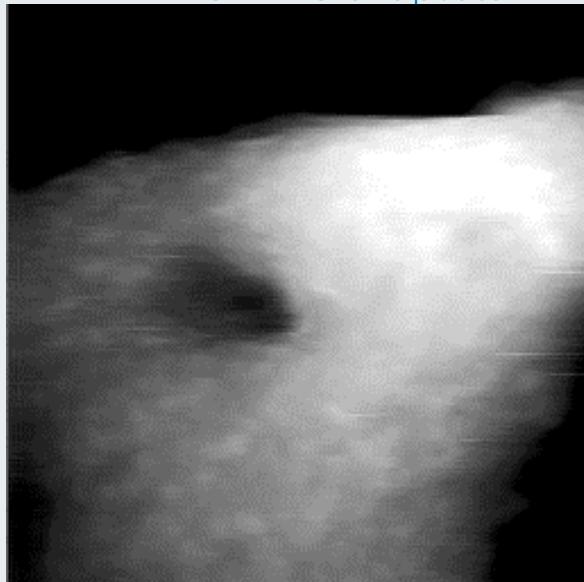
4) Instruments

5) Advanced and novel AFM methods

# High-Speed AFM



ELF3 LLPS droplets

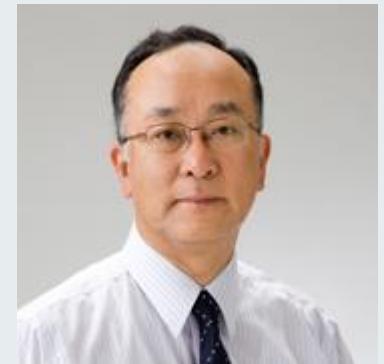


Nessim Louafi

Walking myosin



Toshio Ando

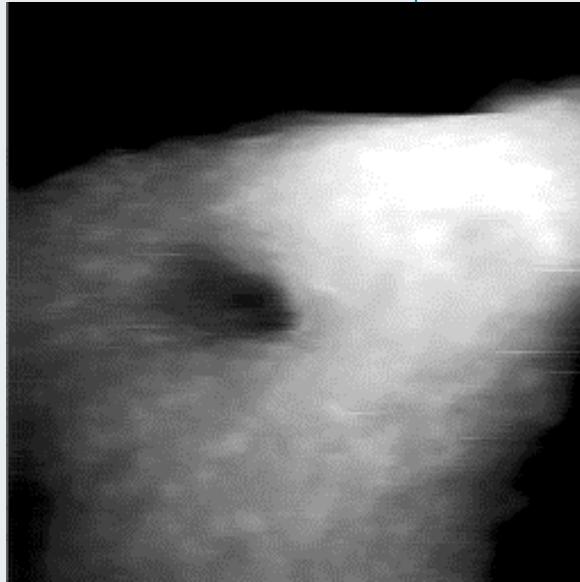


Ando T. et al, PNAS  
98(22), 12468-12472,  
2001

# High-Speed AFM

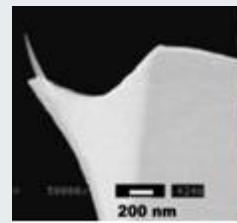
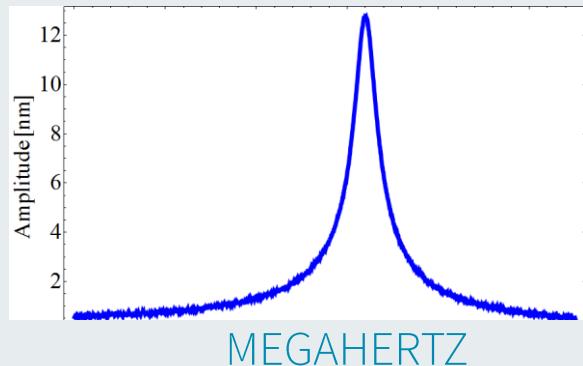


ELF3 LLPS droplets



Nessim Louafi

FAST (SMALL)  
CANTILEVERS



Walking myosin



Toshio Ando



Ando T. et al, PNAS  
98(22), 12468-12472,  
2001

FAST  
XYZ  
SCANNER



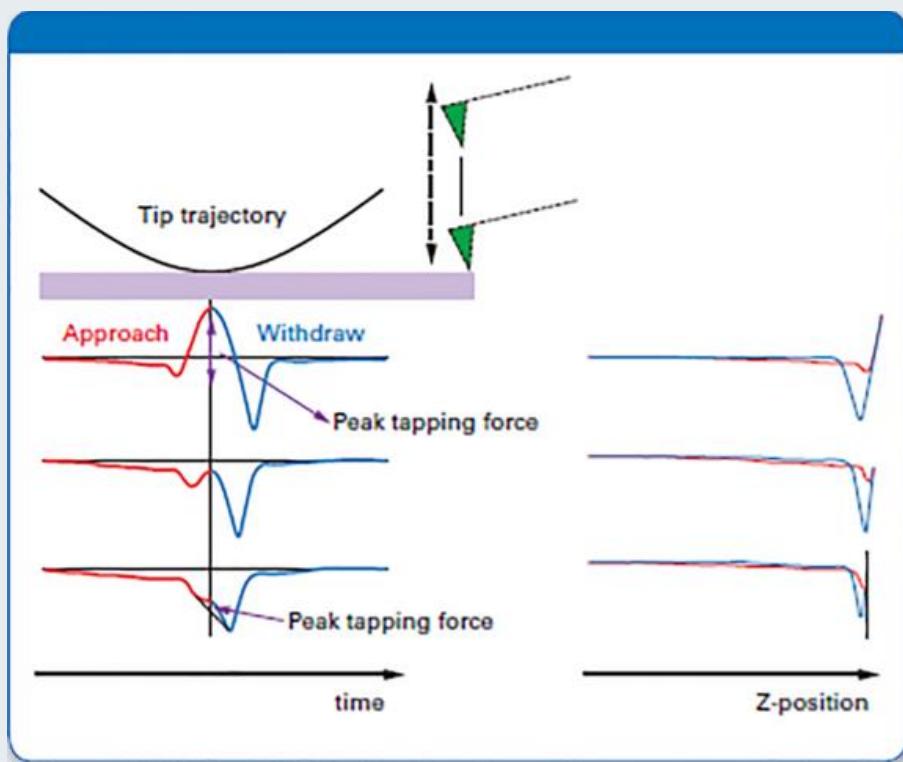
# Fast Force-Curves Imaging



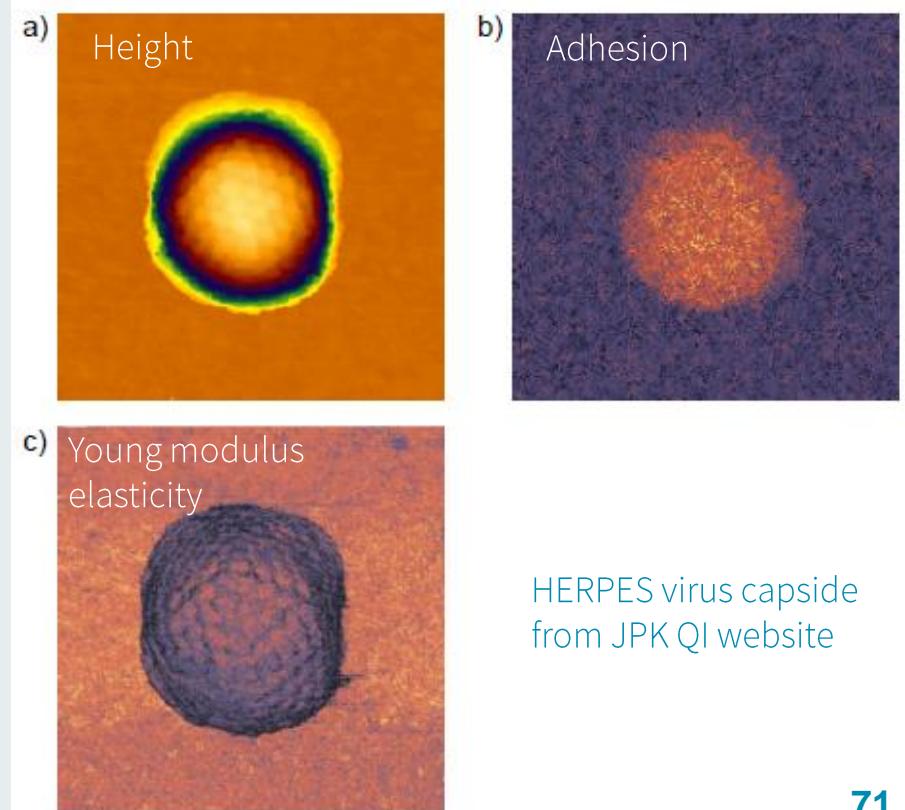
Bruker: PeakForce Tapping

JPK: QI quantitative imaging

Asylum Research: Fast Force Mapping



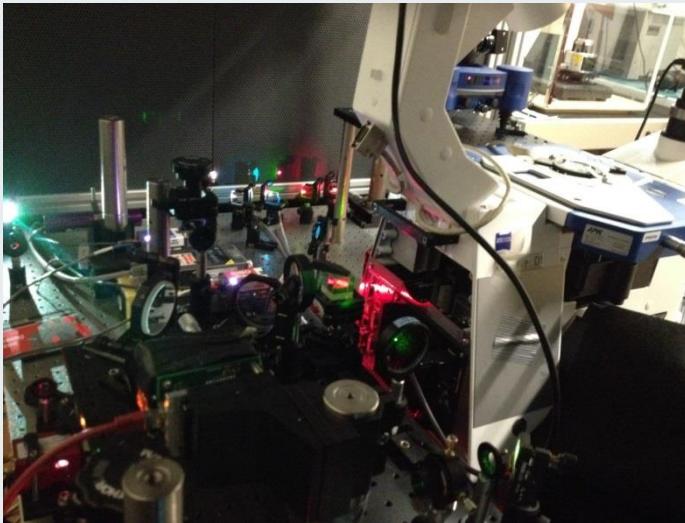
From Bruker website



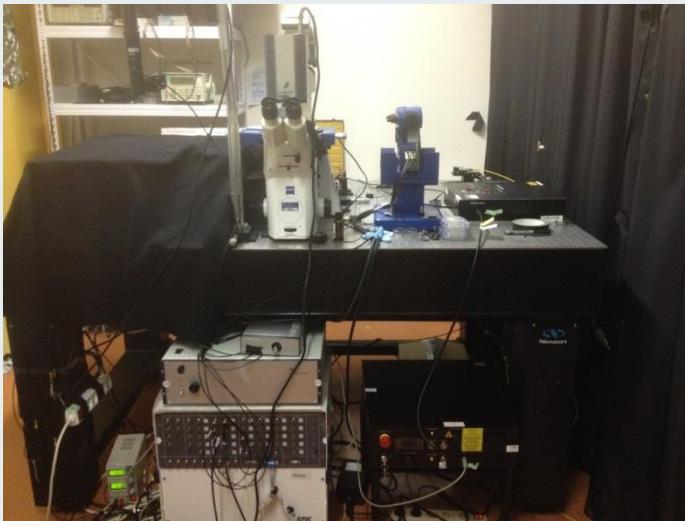
# Correlative AFM - Fluorescence



AFM + Fluorescence → Wide field illumination



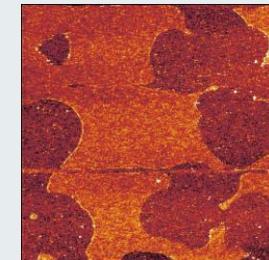
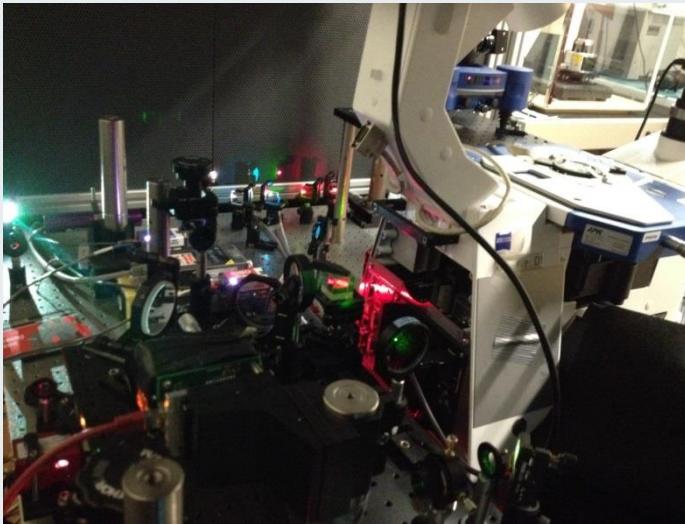
AFM + Fluorescence → Confocal illumination



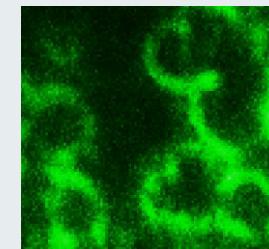
# Correlative AFM - Fluorescence



AFM + Fluorescence → Wide field illumination

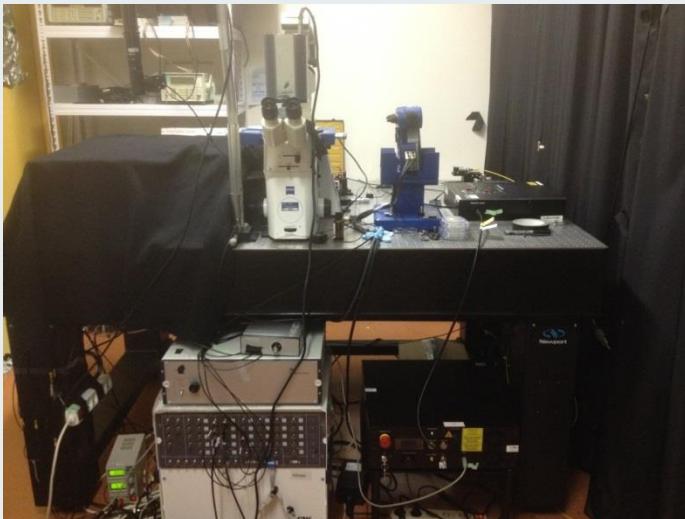


AFM



TIRF  
Fluorescence

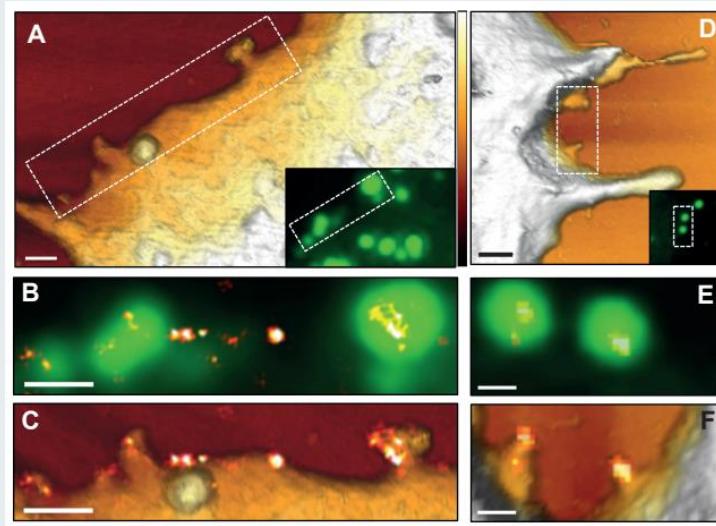
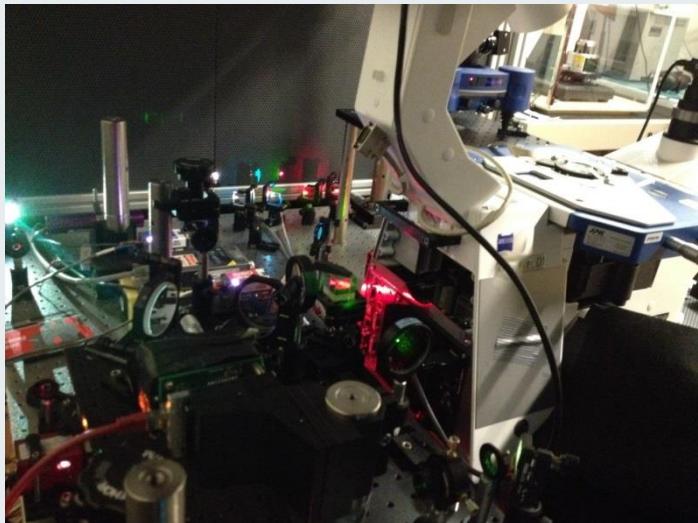
AFM + Fluorescence → Confocal illumination



# Correlative AFM - Fluorescence



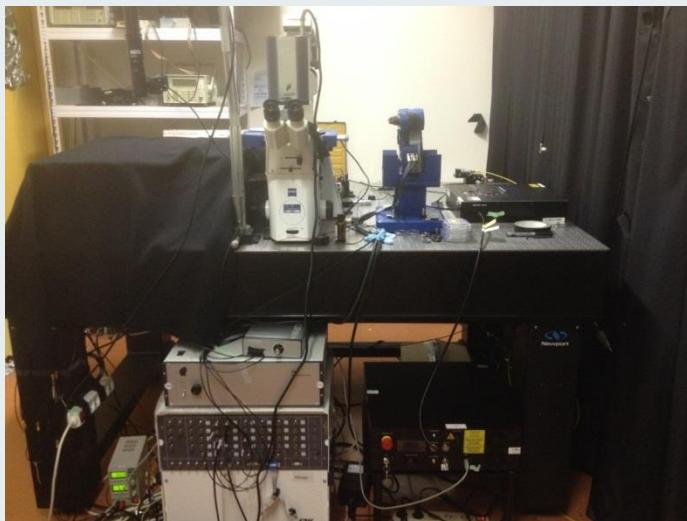
AFM + Fluorescence → Wide field illumination



AFM  
and  
STORM

Dahmane,  
S. et al.,  
Nanoscale,  
2019

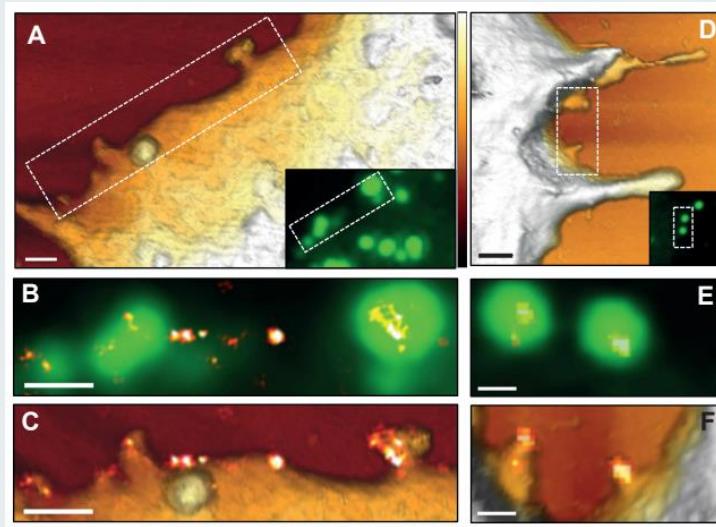
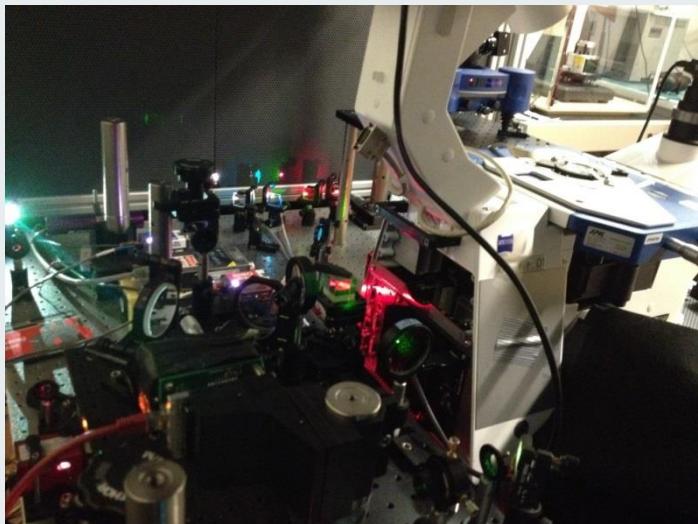
AFM + Fluorescence → Confocal illumination



# Correlative AFM - Fluorescence

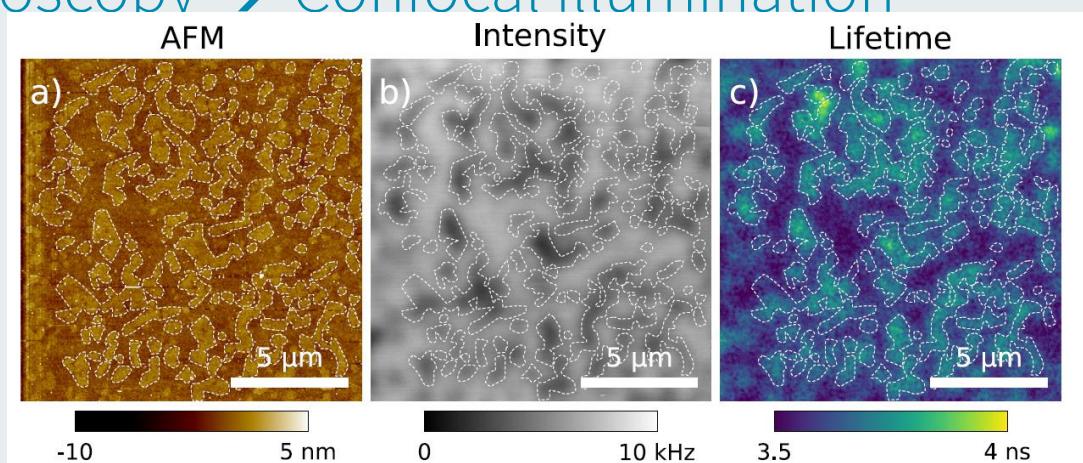
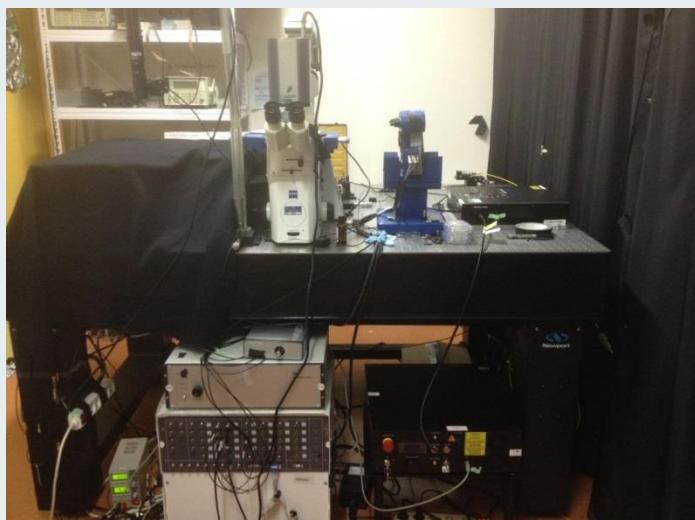


AFM + Fluorescence → Wide field illumination



AFM  
and  
STORM

AFM + Fluorescence Spectroscopy → Confocal illumination



# Tips for High-Resolution AFM imaging



- 1) The instrumental noise should be smaller than the aimed resolution.
- 2) The lateral resolution cannot be smaller than the size of the tip apex.
- 3) The decay length of the tip surface interaction should be smaller than the tip apex.
- 4) Imaging isolated three dimensional objects imposes limits on the lateral resolution.
- 5) The adhesion energy should be minimized. This is usually achieved by using sharp tips.
- 6) The applied force should be as small as possible.
- 7) Under identical conditions (tip radius and applied force), the stiffer the sample the better the lateral resolution.

Ricardo Garcia, Amplitude Modulation Atomic Force Microscopy, Wiley, 2010

Luca Costa  
luca.costa@cbs.cnrs.fr



## Team Integrative Biophysics of Membranes (IBM)

<https://integrativebiophysicsofmembranes.wordpress.com/>

