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NONLOCAL MULTISCALE INTERACTIONS IN BRAIN NEURODEGENERATIVE PROTEIN DYNAMICS AND COUPLED PROTEOPATHIC PROCESSES

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Abstract. We take a heterodimer multiscale reaction-diffusion model as a starting point and modify it to account for the nonlocality of the underlying processes. The resulting model is a coupled system of integro-differential equations. The effect of nonlocal interactions is quantified based on the comparisons of the newly developed model with its local counterpart. Our primary focus is given to the estimation of conversion times from healthy to toxic proteins. This is done based on the stability analysis of a simplified model, as well as on the fully coupled numerical implementation. Several clinically relevant patient proteopathies are highlighted. They include the primary tauopathy, as well as the secondary tauopathy where the sustained presence of toxic tau protein requires also to be accompanied by toxic amyloid-beta peptides. We demonstrate the dynamics of concentrations of toxic proteins under several clinically realistic scenarios. Finally, we carry out a detailed parametric study, providing further insight into the role of nonlinear effects controlled via the Holling type II functional response.

1 INTRODUCTION

In neurodegenerative diseases, a particular intervention based on advanced biomedical engineering is often hindered by our lack of understanding of coupled, concomitant proteinopathies [1]. While there is a continuing debate in the literature about the roles of the proteostasis of amyloid-beta peptides and the microtubule-associated tau protein, it is known that aging alters them both. The processes related to their changes are not independent, they are coupled [2]. Our better understanding of this and other types of

couplings is critical to disease-specific diagnosis, prevention, and treatment of neurodegenerative diseases in general and Alzheimer's disease (AD) in particular [3, 4].

AD is the most common type of neurodegenerative disorder (ND) that increases degrees of dementia over time [5]. It has been reported that 5.5 million Americans in the U.S. and 44 million worldwide deal with this disease in all ranges of ages, while 10% of the population is suffering over 65 years of age [6]. According to the pathological report of AD, one of the main reasons for the loss of nerves and synapses is the accumulation of extracellular amyloid plaques peptides and intracellular neurofibrillary tangles (NFTs) in the nervous system [7, 8]. Generally, tau protein helps to stabilize microtubules within the axon, but when it forms NFTs, it acts as a seed for further misfolding and aggregation. The aggregation of tau proteins happens in the axon and then is transported into extracellular space [9]. Diffusion occurs in that space through secretion and then damage the host cell [10].

The accumulation of these proteins has been studied mathematically [11]. Multiple modes based on differential equations have been used for describing AD. However, a number of questions regarding this disease remain open and more refined models need to be developed to address them. Here, we use a reaction-diffusion equation with a modified heterodimer model in the reaction kinetics to describe the interaction between amyloid-beta and tau protein [11, 12]. In reality, the conversion of healthy protein to toxic protein depends not only on the density located at that spatial location but also on the densities present at the neighbourhood spatial locations. A nonlocal interaction is introduced for capturing such phenomena in the disease propagation. Some relevant clinical tauopathies are discussed in the presence of nonlocal interactions.

2 MATHEMATICAL MODEL

2.1 Local model

We consider $\Omega \subset \mathbb{R}^2$ is a spatial domain. For $x \in \Omega$ and time $t \in \mathbb{R}^+$, we denote by $u = u(\mathbf{x}, t)$ and $v = v(\mathbf{x}, t)$, the concentrations of healthy $A\beta$ and τP respectively. Similarly, we denote by $\tilde{u} = \tilde{u}(\mathbf{x}, t)$ and $\tilde{v} = \tilde{v}(\mathbf{x}, t)$, the concentrations of toxic $A\beta$ and τP respectively. The evolution of concentrations of the four populations can then be given as follows [12]:

$$\frac{\partial u}{\partial t} = \nabla \cdot (\mathbf{D}_1 \nabla u) + a_0 - a_1 u - \frac{a_2 u}{1 + e_1 u} \tilde{u}, \quad (1a)$$

$$\frac{\partial \tilde{u}}{\partial t} = \nabla \cdot (\tilde{\mathbf{D}}_1 \nabla \tilde{u}) - \tilde{a}_1 \tilde{u} + \frac{a_2 u}{1 + e_1 u} \tilde{u}, \quad (1b)$$

$$\frac{\partial v}{\partial t} = \nabla \cdot (\mathbf{D}_2 \nabla v) + b_0 - b_1 v - \frac{b_2 v}{1 + e_2 v} \tilde{v} - b_3 \tilde{u} v \tilde{v}, \quad (1c)$$

$$\frac{\partial \tilde{v}}{\partial t} = \nabla \cdot (\tilde{\mathbf{D}}_2 \nabla \tilde{v}) - \tilde{b}_1 \tilde{v} + \frac{b_2 v}{1 + e_2 v} \tilde{v} + b_3 \tilde{u} v \tilde{v}, \quad (1d)$$

where the first two equations correspond to the usual heterodimer model for the healthy and toxic variants of the protein u and the last two equations are the same for v . Here, a_0 and b_0 are the mean production rates of healthy proteins, a_1, b_1, \tilde{a}_1 and \tilde{b}_1 are the mean clearance rates of healthy and toxic proteins, and a_2 and b_2 represent the mean conversion rates of healthy proteins to toxic proteins. The parameter b_3 is the coupling between the two proteins $A\beta$ and τP . Here, e_1 and e_2 are the dimensionless parameters that describe the conversion time of the healthy protein to the toxic protein of $A\beta$ and τP , respectively. The diffusion tensors $\mathbf{D}_1, \tilde{\mathbf{D}}_1, \mathbf{D}_2$ and $\tilde{\mathbf{D}}_2$ characterize the spreading of each proteins. We assume all variables and initial conditions to be non-negative, and all the parameters to be strictly positive.

2.2 Nonlocal model

In model (1), the conversion of toxic protein from the healthy protein at a spatial point \mathbf{x} depends only on the healthy proteins located at the same spatial point \mathbf{x} . In general, the converted toxic protein located at a spatial point \mathbf{x} depends on the healthy proteins located in the neighbourhood of the spatial point \mathbf{x} . Under this assumption, we modify the model (1), inspired by the ideas presented in [13]:

$$\frac{\partial u}{\partial t} = \nabla \cdot (\mathbf{D}_1 \nabla u) + a_0 - a_1 u - \frac{a_2 u}{1 + e_1 u} \Phi * \tilde{u}, \quad (2a)$$

$$\frac{\partial \tilde{u}}{\partial t} = \nabla \cdot (\tilde{\mathbf{D}}_1 \nabla \tilde{u}) - \tilde{a}_1 \tilde{u} + a_2 \tilde{u} \Phi * \left(\frac{u}{1 + e_1 u} \right), \quad (2b)$$

$$\frac{\partial v}{\partial t} = \nabla \cdot (\mathbf{D}_2 \nabla v) + b_0 - b_1 v - b_3 \tilde{u} v \tilde{v} - \frac{b_2 v}{1 + e_2 v} \Phi * \tilde{v} \quad (2c)$$

$$\frac{\partial \tilde{v}}{\partial t} = \nabla \cdot (\tilde{\mathbf{D}}_2 \nabla \tilde{v}) - \tilde{b}_1 \tilde{v} + b_3 \tilde{u} v \tilde{v} + b_2 \tilde{v} \Phi * \left(\frac{v}{1 + e_2 v} \right), \quad (2d)$$

where the convolution $\Phi * \tilde{u}$ is defined by $(\Phi * \tilde{u})(\mathbf{x}, t) = \int_{\Omega} \Phi(\mathbf{x} - \mathbf{y}) \tilde{u}(\mathbf{y}, t) d\mathbf{y}$ with $\int_{\Omega} \Phi(\mathbf{x}) d\mathbf{x} = 1$. Similarly, we define the other convolutions. Here, Φ is the kernel functions that describe the conversion efficiencies between the spatial points \mathbf{x} and \mathbf{y} . In this work, we use the following Gaussian kernel function [14]:

$$\phi(\mathbf{x}) = \frac{1}{\sigma \sqrt{\pi}} \exp\left(-\frac{\mathbf{x} \cdot \mathbf{x}}{\sigma^2}\right). \quad (3)$$

2.3 Network model

Here, we describe a nonlocal network mathematical model corresponding to the non-local continuous model (2) and accounting for the brain data. The brain connectome can be modelled by a coarse-grain model of the continuous system. It is a weighted graph \mathcal{G} with V nodes and E edges defined in a domain Ω . Specifically, it can be considered as weights of the graph \mathcal{G} is represented by the adjacency matrix \mathbf{W} and helps to construct

the graph of the Laplacian. For $i, j = 1, 2, 3, \dots, V$, the elements of \mathbf{W} are

$$W_{ij} = \frac{n_{ij}}{l_{ij}^2},$$

where n_{ij} is the mean fiber number and l_{ij}^2 is the mean length squared between the nodes i and j . We define the graph of the Laplacian \mathbf{L} as

$$L_{ij} = \rho(D_{ii} - W_{ij}), \quad i, j = 1, 2, 3, \dots, V,$$

where ρ is the diffusion coefficient and $D_{ii} = \sum_{j=1}^V W_{ij}$ is the elements of the diagonal weighted degree matrix.

Likewise, similar to the nonlocal continuous PDE model (2), we define the nonlocal conversion for the network model for each of the nodes $j = 1, 2, 3, \dots, V$. For a fixed node j , we first find all the nodes $V_{j,1}$ directly connected to the node j . Similarly, we find the immediate connecting nodes $V_{j,2}$ connected with the nodes $V_{j,1}$ and so on. In this way, we find all the sets of nodes $V_{j,1}, V_{j,2}, \dots, V_{j,m_j}$ connected with the node j . Now, we sort all the nodes $V_{j,1}$ according to minimum distances from the node j and labelled as $V_{j,1}^s$. Similarly, we sort all the set of nodes $V_{j,2}, V_{j,3}, \dots, V_{j,m_j}$ according to shortest distances from the node j through the edges and labelled as $V_{j,2}^s, V_{j,3}^s, \dots, V_{j,m_j}^s$. Suppose, n_j is the total number of nodes connected with the node j including the self node j and k_1, k_2, \dots, k_{n_j} are the new labelled of the sorted connected nodes starting with the self node j i.e., $k_1 = j$. We define a set of n_j elements of weights as

$$M'_j = \left\{ 1, e^{-\eta^2(s_{jk_2})^2}, e^{-\eta^2(s_{jk_3})^2}, \dots, e^{-\eta^2(s_{jk_{n_j}})^2} \right\},$$

where s_{jk_i} denotes the shortest distance from the node k_i to the node j along the edges and $\eta = 1/\sigma$.

We normalize M'_j as $M_j = M'_j/|M'_j|$, where

$$|M'_j| = \left(1 + e^{-\eta^2(s_{jk_2})^2} + e^{-\eta^2(s_{jk_3})^2} + \dots + e^{-\eta^2(s_{jk_{n_j}})^2} \right).$$

Now, we define a row vector C_j of V number of elements with non-zero elements being $M_j(1), M_j(2), \dots, M_j(n_j)$ at the indices k_1, k_2, \dots, k_{n_j} respectively. Finally, we are ready to define the convolution at the node j in the graph \mathcal{G} as

$$\Phi_j * \tilde{u}_j = \sum_{n=1}^V C_j(n) \tilde{u}_n.$$

If the node j is not connected with the other nodes, then $\Phi_j * \tilde{u}_j = \tilde{u}_j$. Similarly, we define the other convolutions.

Taking into account all the factors (Laplacian and convolutions), we build a nonlocal network mathematical model on the graph \mathcal{G} . At the node j , let (u_j, \tilde{u}_j) be the concentrations of healthy and toxic $A\beta$ and (v_j, \tilde{v}_j) be the concentrations of healthy and toxic τP , respectively. Then for all the nodes $j = 1, 2, 3, \dots, V$, the network equations corresponding to the continuous model (2) is a system of first order differential equations and it is given by

$$\frac{du_j}{dt} = - \sum_{k=1}^V L_{jk} u_k + a_0 - a_1 u_j - \frac{a_2 u_j}{1 + e_1 u_j} \Phi_j * \tilde{u}_j, \quad (4a)$$

$$\frac{d\tilde{u}_j}{dt} = - \sum_{k=1}^V L_{jk} \tilde{u}_k - \tilde{a}_1 \tilde{u}_j + a_2 \tilde{u}_j \Phi_j * \left(\frac{u_j}{1 + e_1 u_j} \right), \quad (4b)$$

$$\frac{dv_j}{dt} = - \sum_{k=1}^V L_{jk} v_k + b_0 - b_1 v_j - b_3 \tilde{u}_j v_j \tilde{v}_j - \frac{b_2 v_j}{1 + e_2 v_j} \Phi_j * \tilde{v}_j, \quad (4c)$$

$$\frac{d\tilde{v}_j}{dt} = - \sum_{k=1}^V L_{jk} \tilde{v}_k - \tilde{b}_1 \tilde{v}_j + b_3 \tilde{u}_j v_j \tilde{v}_j + b_2 \tilde{v}_j \Phi_j * \left(\frac{v_j}{1 + e_2 v_j} \right), \quad (4d)$$

with non-negative initial conditions.

2.4 Homogeneous stationary solution

Before analysing the full nonlocal model, we first study its temporal and local dynamics. The stationary points of the temporal model are the homogeneous stationary solutions of the local model. Here, the system has at least one stationary solution called the trivial stationary solution and is given by

$$(u_1, \tilde{u}_1, v_1, \tilde{v}_1)(\mathbf{x}) = \left(\frac{a_0}{a_1}, 0, \frac{b_0}{b_1}, 0 \right). \quad (5)$$

Depending on the parameter values, the system may have non-trivial stationary solutions. We list all of them in the below.

1. Healthy $A\beta$ - toxic τP : The stationary solution corresponding to healthy $A\beta$ - toxic τP is given by

$$(u_2, \tilde{u}_2, v_2, \tilde{v}_2)(\mathbf{x}) = \left(\frac{a_0}{a_1}, 0, \frac{\tilde{b}_1}{b_2 - e_2 \tilde{b}_1}, \frac{b_0(b_2 - e_2 \tilde{b}_1) - b_1 \tilde{b}_1}{\tilde{b}_1(b_2 - e_2 \tilde{b}_1)} \right). \quad (6)$$

For the non-negativity of the stationary solution (6), we must have $b_2 > e_2 \tilde{b}_1$ and $b_0/b_1 \geq \tilde{b}_1/(b_2 - e_2 \tilde{b}_1)$.

2. Toxic $A\beta$ - healthy τP : The stationary solution corresponding to toxic $A\beta$ - healthy τP is given by

$$(u_3, \tilde{u}_3, v_3, \tilde{v}_3)(\mathbf{x}) = \left(\frac{\tilde{a}_1}{a_2 - e_1 \tilde{a}_1}, \frac{a_0(a_2 - e_1 \tilde{a}_1) - a_1 \tilde{a}_1}{\tilde{a}_1(a_2 - e_1 \tilde{a}_1)}, \frac{b_0}{b_1}, 0 \right). \quad (7)$$

For the non-negativity of the stationary solution (7), we must have $a_2 > e_1 \tilde{a}_1$ and $a_0/a_1 \geq \tilde{a}_1/(a_2 - e_1 \tilde{a}_1)$.

3. Toxic $A\beta$ - toxic τP : Suppose $(u_4, \tilde{u}_4, v_4, \tilde{v}_4)(\mathbf{x})$ is a stationary solution of the “toxic $A\beta$ - toxic τP ” type. Here, we have $u_4 = u_3$, $\tilde{u}_4 = \tilde{u}_3$, $\tilde{v}_4 = (b_0 - b_1 v_4)/\tilde{b}_1$ and v_4 satisfy the quadratic equation

$$b_3 e_2 \tilde{u}_4 v_4^2 + (b_3 \tilde{u}_4 - e_2 \tilde{b}_1 + b_2) v_4 - \tilde{b}_1 = 0. \quad (8)$$

The equation (8) always has a real positive solution. For the uniqueness of v_4 , we must have $b_3 \tilde{u}_4 - e_2 \tilde{b}_1 + b_2 \geq 0$. Also, for the positivity of \tilde{v}_4 , we need $v_4 < b_0/b_1$.

3 RESULTS AND DISCUSSION

Here, we study two fundamental disease propagation modes for the local and nonlocal models depending on the parameter values: (i) primary tauopathy and (ii) secondary tauopathy. For the case of primary tauopathy, the toxic τP can exist independently from $A\beta$ concentration, whereas the τP does not exist for the secondary tauopathy. We study these two tauopathies for the network model corresponding to both the local and nonlocal models in the brain connectome. Here, we have considered a high-resolution brain connectome structure consisting of 1,015 vertices and 70,892 edges; the data source is freely available by patients connectome data (<https://braingraph.org>). All the computations are done by using C programming language and Matlab.

Table 1: Fixed parameter values

$A\beta$ system parameters	τP system parameters
$a_0 = 0.75$	$b_0 = 0.5$
$a_1 = 1.0$	$b_1 = 1.0$
$a_2 = 1.0$	$b_2 = 1.0$
$\tilde{a}_1 = 0.6$	$\tilde{b}_1 = 0.4$

We apply the local and nonlocal versions of (4) to a computational case for Alzheimer’s disease. In particular, we consider seeding sites for toxic $A\beta$ and toxic τP proteins associated with Alzheimer’s disease staging. Alzheimer’s disease is a multiscale phenomenon. A uniform parameter value can be considered throughout all the regions in the brain

or different values in different regions depending on the patient's disease progression. Initially, we investigate the primary and secondary tauopathies by considering simple uniform parameter values in all the regions. We choose the uniform parameters for both the tauopathies from Table 1.

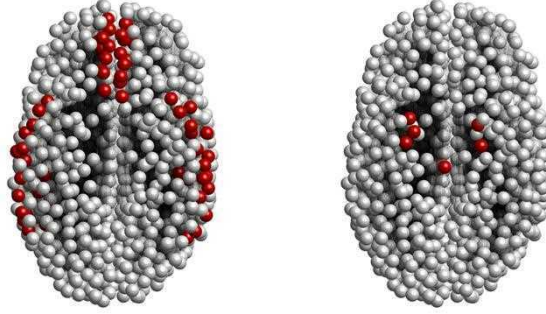


Figure 1: (Color online) Seeding sites for Alzheimer's disease: (left) toxic $A\beta$ and (right) toxic τP .

The seeding sites of toxic $A\beta$ protein associated with Alzheimer's disease are the temporobasal and frontomedial regions [11, 15, 16, 17, 18]. On the other hand, the tau staging for the AD begins in the locus coeruleus and transentorhinal regions [11, 15, 17, 18], as follows from [19]. Seeding sites for toxic $A\beta$ and toxic τP are shown in the left and right respectively in Fig. 1, and their regions are highlighted by red color.

3.1 Primary tauopathy

For the primary tauopathy, we take all the parameters mentioned in Table 1 with the coupling parameter $b_3 = 1$. Here, all the stationary solutions (5)-(8) exist. Initially, we set all the nodes in the brain connectome being healthy, but all are assumed to be susceptible. Therefore, the primary tauopathy state is the "healthy $A\beta$ - healthy τP " state i.e., $(u_1, \tilde{u}_1, v_1, \tilde{v}_1) = (0.75, 0, 0.5, 0)$. For the seeding sites of toxic $A\beta$, i.e., the temporobasal and frontomedial regions, initially we deviate 1% concentration of healthy concentration. Similarly, for the toxic τP , we perturb 1% of healthy concentration of τP in the locus coeruleus and transentorhinal regions.

We first study the disease propagation by using the local network model. Brain-wide spatial averages of all the four protein populations at each time instance are shown in Fig. 2. The disease propagation is shown for four different values of e_1 and e_2 . We also plot the propagation of toxic tau protein in the brain connectome for $e_1 = e_2 = 0$ and $e_1 = e_2 = 0.1$ in Fig. 3. For simplicity, we choose $e_1 = e_2$. For higher values of e_1 and e_2 , the local network model takes a long time to propagate the disease over the brain connectome. Therefore, the introduction of reaction time (described by the Holling type-II functional response) increases the invasion time window for propagating AD over

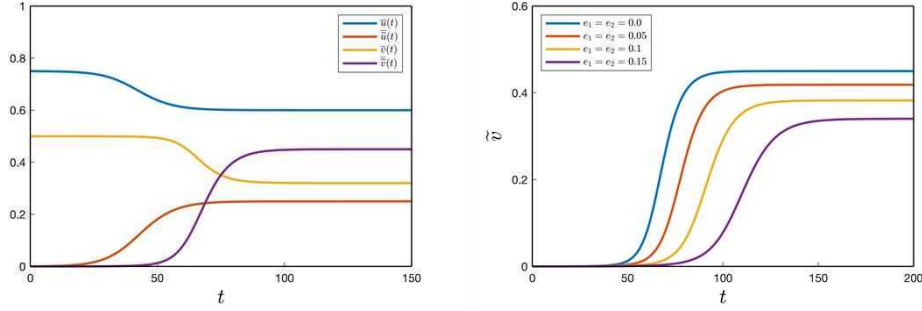


Figure 2: (Color online) Brain-wide spatial averages of the protein populations: (left) all four populations with $e_1 = e_2 = 0$ and (right) toxic - τP with different $e_1 (= e_2)$.

the brain. It reduces the overall toxic level in the brain as well.

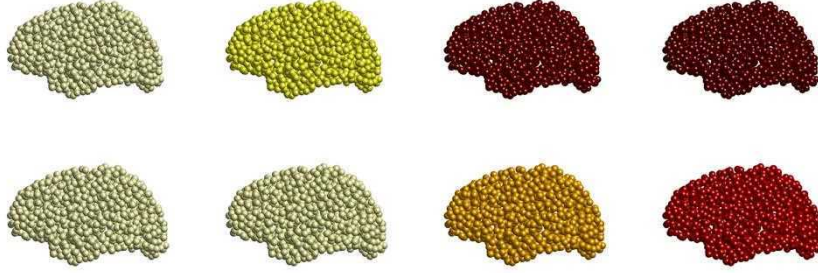


Figure 3: (Color online) Toxic τP propagation in the brain connectome at different time instances: (left to right) $t = 30, 60, 90$ and 120 ; Upper and lower panels are corresponding to $e_1 = e_2 = 0$ and $e_1 = e_2 = 0.1$, respectively.

3.2 Secondary tauopathy

For the secondary tauopathy, we take the parameters from Table 1 except the parameter $b_2 = 0.75$ and we choose the coupling parameter $b_3 = 3$. In this case, the stationary solution (6) does not exist. We set all the nodes healthy but susceptible, and the initial condition is the same as for primary tauopathy [see Fig. 1]. The invaded concentrations of the four populations for the secondary tauopathy is the “toxic $A\beta$ - toxic τP ” state. The spreading patterns for the secondary tauopathy are similar to those of the primary tauopathy.

In both the tauopathies, the spreading patterns for the local and nonlocal models are the same. Their concentrations are also the same. This is due to the uniform parameter values all over the regions in the brain connectome. With the increase in the shortest distance between the connecting nodes, the weight-age of the nonlocal effect decreases exponentially. We have observed that the nonlocal interactions do not affect qualitatively

the uniform parameter values over all the regions of the brain connectome. Now, we see the impact of nonlocal interactions on the results when the system has different parameter values in different regions of the brain connectome.

3.3 Mixed tauopathies with non-uniform parameters

Till now, we have considered some general features of the two tauopathies with synthetic and global constant parameter values. On the other hand, the positron emission tomography (PET) imaging studies of $A\beta$ and τP radiotracer uptake provide us with additional insight. The distribution of PET- τP SUVR intensities in Alzheimer's disease is biased towards the brain's temporal and parietal regions. These features are absent in the previous two tauopathies. Now, we study the model local and nonlocal effects with network system (4) along with the Alzheimer's disease patient data. A sample data is taken from the Alzheimer's Disease Neuroimaging Initiative (ADNI) database [11].

Table 2: General synthetic parameters values

Healthy $A\beta$	Toxic $A\beta$	Healthy τP	Toxic τP
$\rho = 1.38$	$\rho = 0.138$	$\rho = 1.38$	$\rho = 0.014$
$a_0 = 1.035$	$\tilde{a}_1 = 0.828$	$b_0 = 0.69$	$\tilde{b}_1 = 0.552$
$a_1 = 1.38$	$a_2 = 1.38$	$b_1 = 1.38$	$b_2 = 1.035$

Table 3: Modified b_3 values

Brain region ID and modified b_3 value			
Pars Opercularis	7.452	Rostral middle frontal gyrus	6.707
Superior frontal gyrus	7.452	Caudal middle frontal gyrus	7.452
Precentral gyrus	5.589	Postcentral gyrus	3.726
Lateral orbitofrontal cortex	6.486	Medial orbitofrontal cortex	6.486
Pars triangularis	5.520e-6	Rostral anterior cingulate	6.210e-6
Posterior cingulate cortex	3.45	Inferior temporal cortex	13.11
Middle temporal gyrus	11.04	Superior temporal sulcus	8.97
Superior temporal gyrus	8.28	Superior parietal lobule	12.42
Cuneus	13.8	Pericalcarine cortex	13.8
Inferior parietal lobule	11.73	Lateral occipital sulcus	15.18
Lingual gyrus	13.8	Fusiform gyrus	7.59
Parahippocampal gyrus	11.04	Temporal pole	1.104e-5

First, we set all regions in the connectome to a state of secondary tauopathy with the general synthetic parameters given in Table 2 with $b_3 = 4.14$. The coupling parameter b_3 is modified in several regions [see Table 3]. This modification is symmetric, i.e., b_3 has the same value for both the left and right hemispheres in the corresponding regions. We also modify b_2 and b_3 in some of the regions, and in this case, the system has a state of primary tauopathy [see Table 4]. After combining all the modified values, the system came up with a mixed state of tauopathy, i.e., a state of primary and secondary tauopathies exist simultaneously in different regions of the brain connectome.

Table 4: Modified b_2 and b_3 values

Brain region	Entorhinal cortex	Pallidum	Locus coeruleus	Putamen	Precuneus
b_2	3.125	2.76	1.38	3.795	3.105
b_3	1.104e-5	2.76	1.38	3.795	3.105

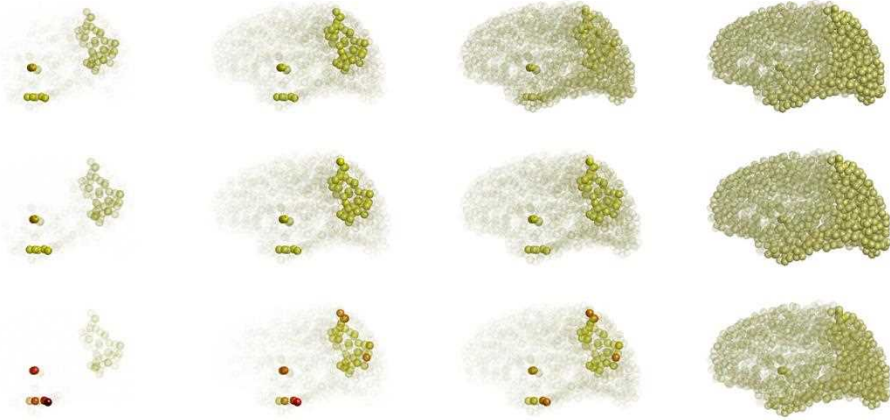


Figure 4: (Color online) Toxic τP propagation in the brain connectome at different time instances: (left to right) $t = 20, 30, 50$ and 100 ; Upper panel is corresponding to the local model; Middle and lower panels are corresponding to the nonlocal model with $\eta = 0.5$ and $\eta = 0.25$, respectively.

We solve the local and nonlocal variants network model (4) with the modified regional parameter values. The seeding sites of toxic $A\beta$ and τP are mentioned earlier [see Fig. 1]. Toxic τP propagation in the brain connectome for both the local and nonlocal versions are shown in Fig. 4 at $t = 20, 30, 50$ and 100 . The solution at $t = 100$ is stationary, i.e.,

it remains the same for large values t . In this case, non-uniform concentrations of all four populations exist. This is true because the concentrations of toxic $A\beta$ and toxic τP are not uniformly distributed in the real brain. We also see that the spreading patterns for both the local and nonlocal models are different for the mixed tauopathy.

4 CONCLUSION

We have considered a modified version of coupled heterodimer multiscale model for better understanding the dynamics of Alzheimer's disease. The network-based model corresponding to a PDE system is studied. For the first time, we have introduced nonlocal interactions into the considered network model. Two types of tauopathies (primary and secondary) are discussed separately, and their mixed tauopathy is also analysed. We have concluded that the spreading patterns and the invasion time windows for the local and nonlocal models for both the tauopathies are the same for the uniform parameters in all the regions of the brain connectome. However, the spreading patterns for the local and nonlocal models are different when mixed types of tauopathy are considered. Hence, the introduction of nonlocal interactions makes important qualitative changes in spreading all the four proteins over the brain.

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