



Centre for Medical Image Computing  
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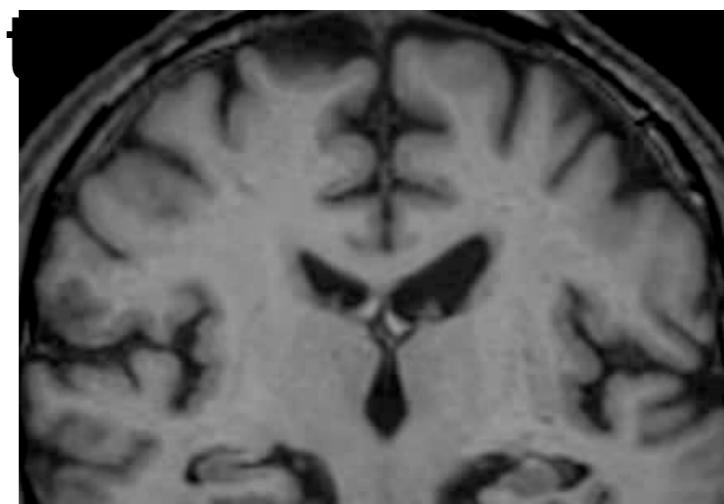


Dementia  
Research  
Centre

# Medical Image Registration Advanced

*Marc Modat*

Centre for Medical Image Computing  
Dementia Research Centre  
**University College London**



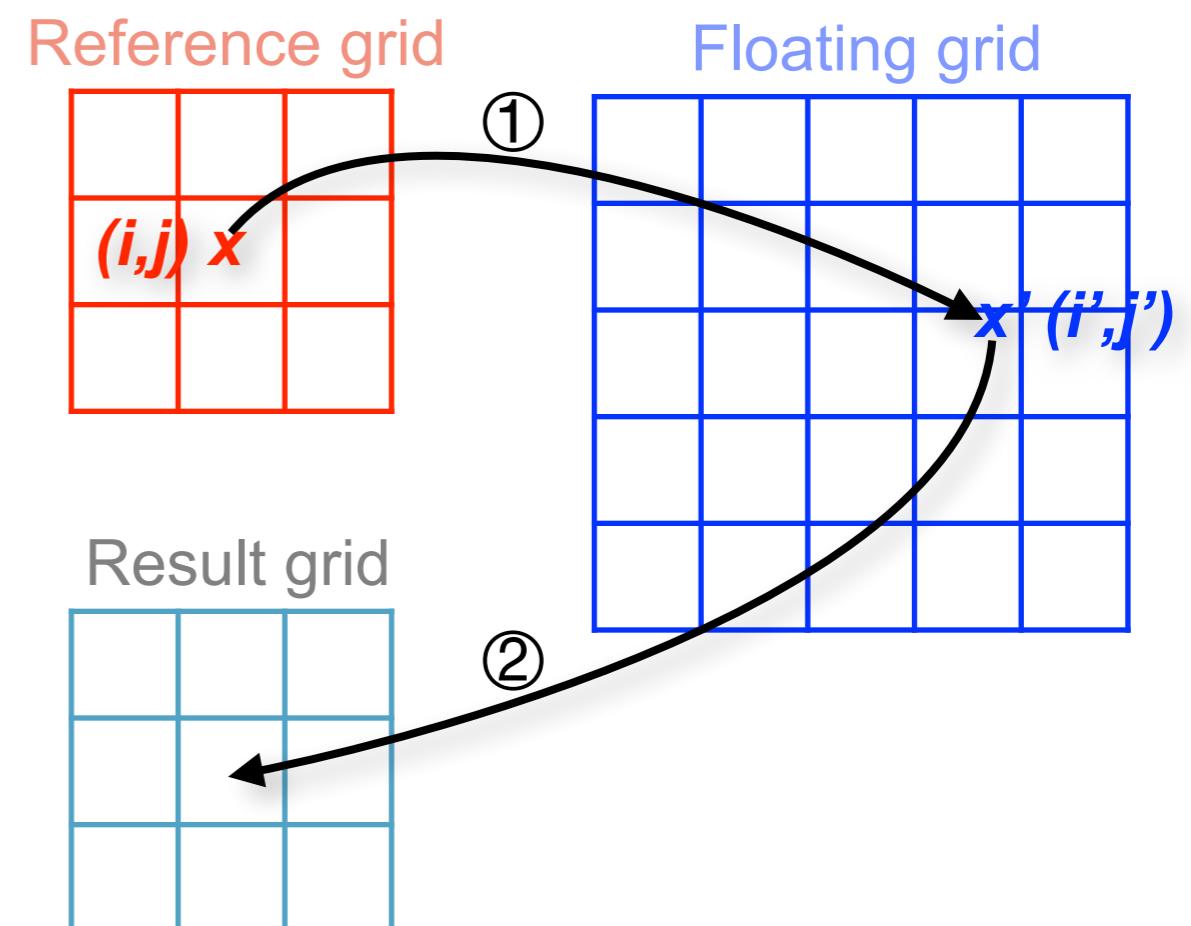
# Outline

- Focus is on transformation parametrisation
  - Deformation field composition, application to:
    - The demons algorithm (1996)
    - Regridding
      - » The fluid algorithm (1996)
      - » The FFD algorithm (2006)
  - Velocity field parametrisation
    - Concept
      - » The Euler integration
      - » The scaling-and-squaring approach (2006)
    - Stationary velocity field
      - » The demons (2009)
      - » The Dartel (2007)
    - Non-stationary velocity field
      - » The LDDMM (2005)

# Reminder on deformation field

① For each pixel with coordinate  $(i, j)$  in the reference image, we know the corresponding position  $(i', j')$  in the floating image.

② In order to deform the floating image, the intensity at position  $(i', j')$  is evaluated using resampling technique and displayed in the result image.



# Def. field composition - Principle

- Simple transformation

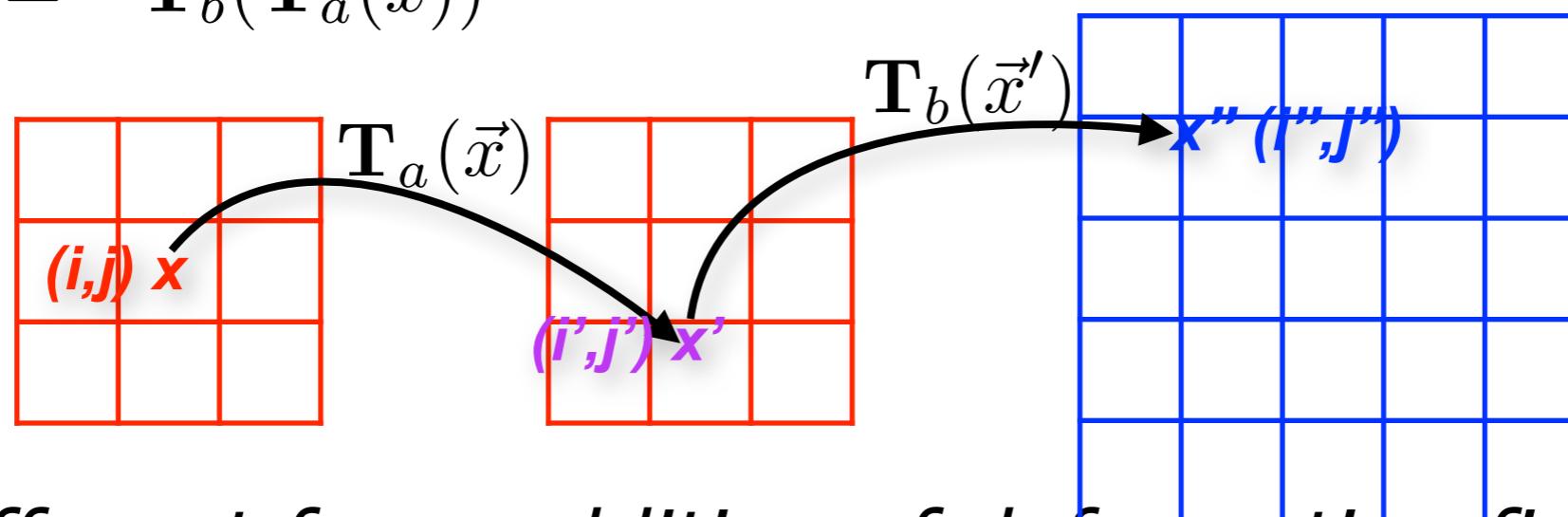
$\mathbf{T}(\vec{x}) = \vec{x}'$ , where  $\vec{x} = \{i, j\}$  and  $\vec{x}' = \{i', j'\}$

- Composition of 2 transformations  $\mathbf{T}_a$  and  $\mathbf{T}_b$  to generate a third one

$\mathbf{T}_c$

$\mathbf{T}_a(\vec{x}) = \vec{x}'$  and then  $\mathbf{T}_b(\vec{x}') = \vec{x}''$ ,

$\mathbf{T}_c(\vec{x}) = \mathbf{T}_b(\mathbf{T}_a(\vec{x}))$

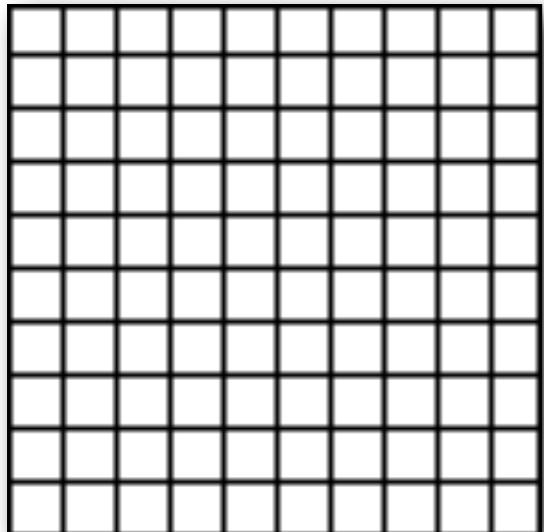


- !!!!!! Different from addition of deformation field

# Def. field composition - Illustration

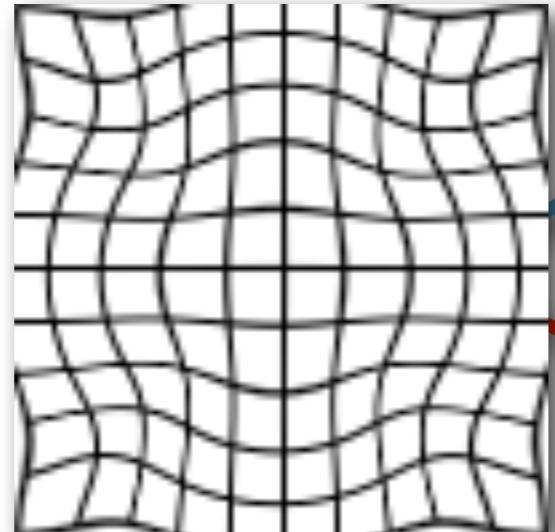
- Composition versus addition of transformation

$$\vec{x} = \vec{x}'$$



*no deformation*

$$\mathbf{T}(\vec{x}) = \vec{x}'$$



*deformed grid*

*Composition*

$$\mathbf{T}(\mathbf{T}(\mathbf{T}(\mathbf{T}(\vec{x})))) = \vec{x}'$$



*Addition*

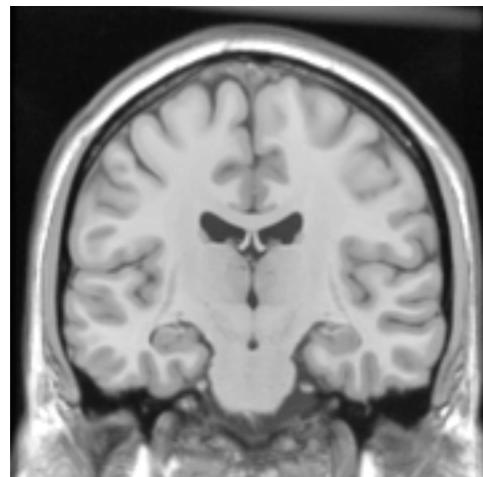
$$\vec{x} + 4 \times (\mathbf{T}(\vec{x}) - \vec{x}) = \vec{x}'$$



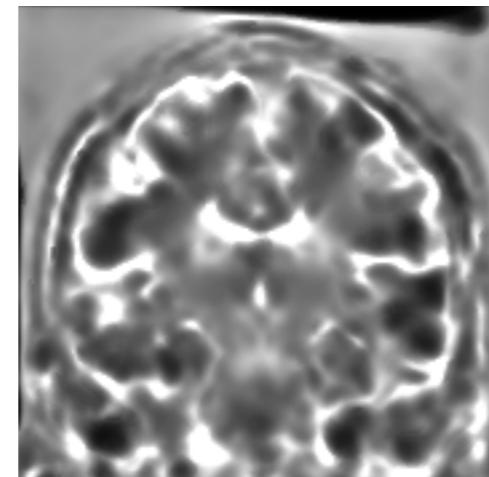
# Def. field composition - Advantages

- The composition of two diffeomorphisms is a diffeomorphism
  - One-to-one mapping
  - The topology is conserved
  - The transformation is invertible

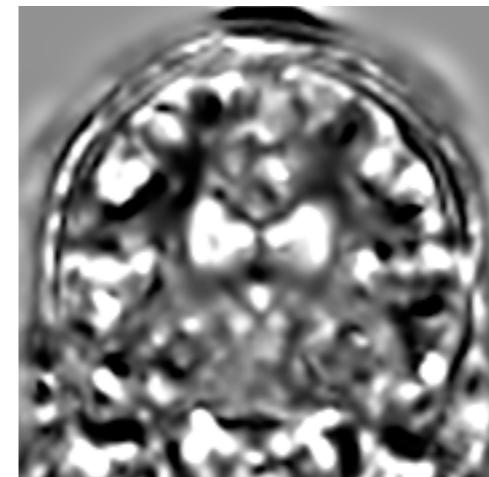
*Jacobian determinant, visualisation scale: [0;2]*



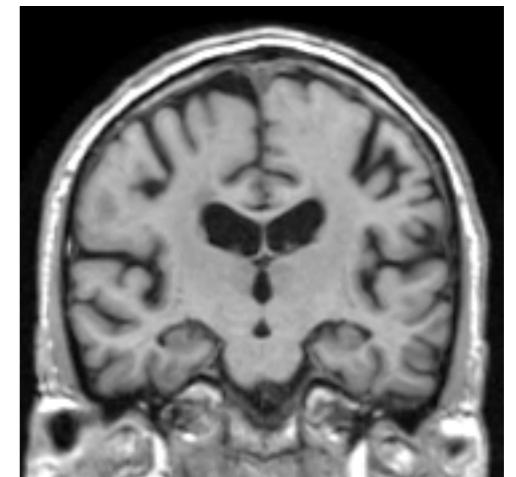
*Reference*



*Composition*  
*Robust range*  
[0.25;2.32]



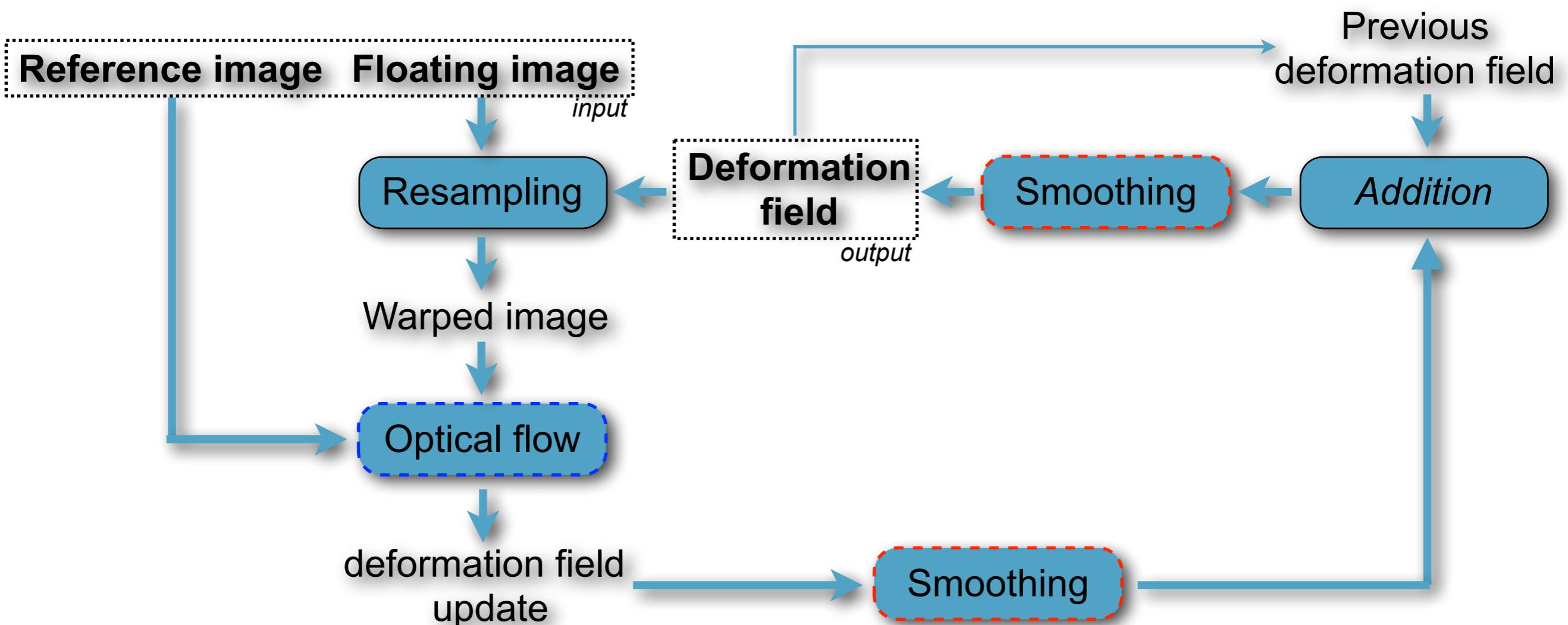
*Addition*  
*Robust range*  
[-0.01;2.95]



*Floating*

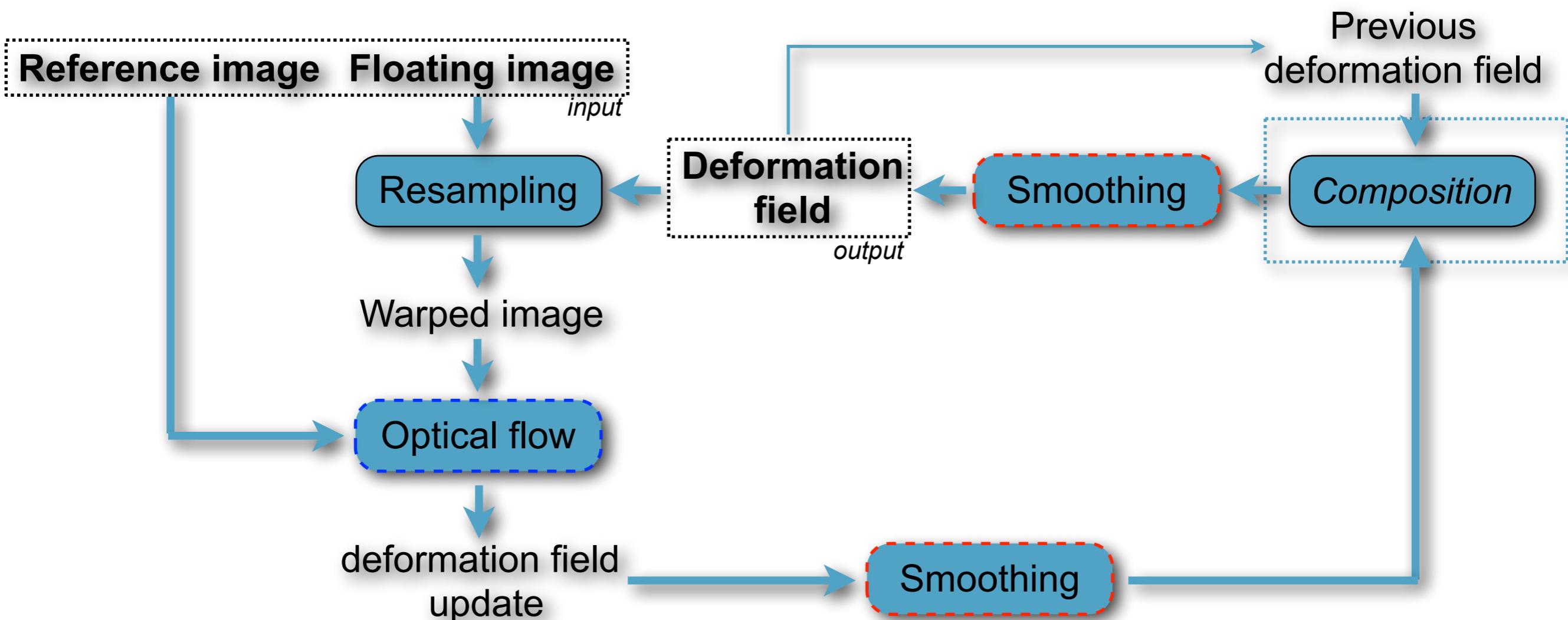
# Demons algorithm

- From the additive demon algorithm to the diffeomorphic version
  - Additive version (introduced during the previous lecture):



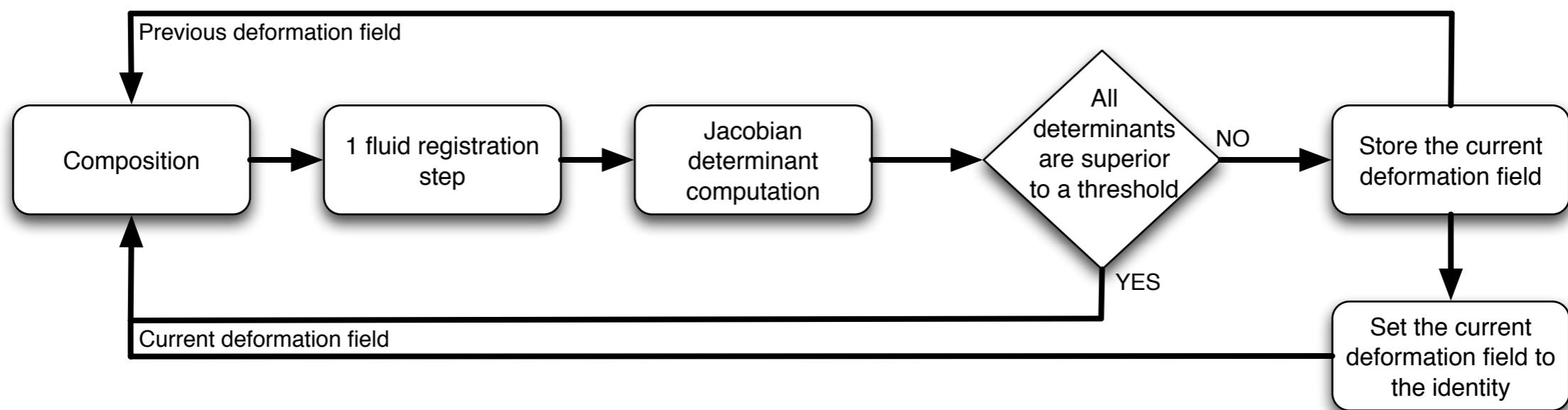
# Demons algorithm

- From the additive demon algorithm to the diffeomorphic version
  - Diffeomorphic version (with constraint on the update):



# Regridding (Jac. det. monitoring)

- Example of application: regridding applied to the fluid algorithm



- Current grid is initialised to identity transformation
- Regridding avoid negative Jacobian determinant using appropriate threshold value.

# Regridding (Hard constraint)

- Example of application: regridding applied to a cubic B-Spline parametrisation

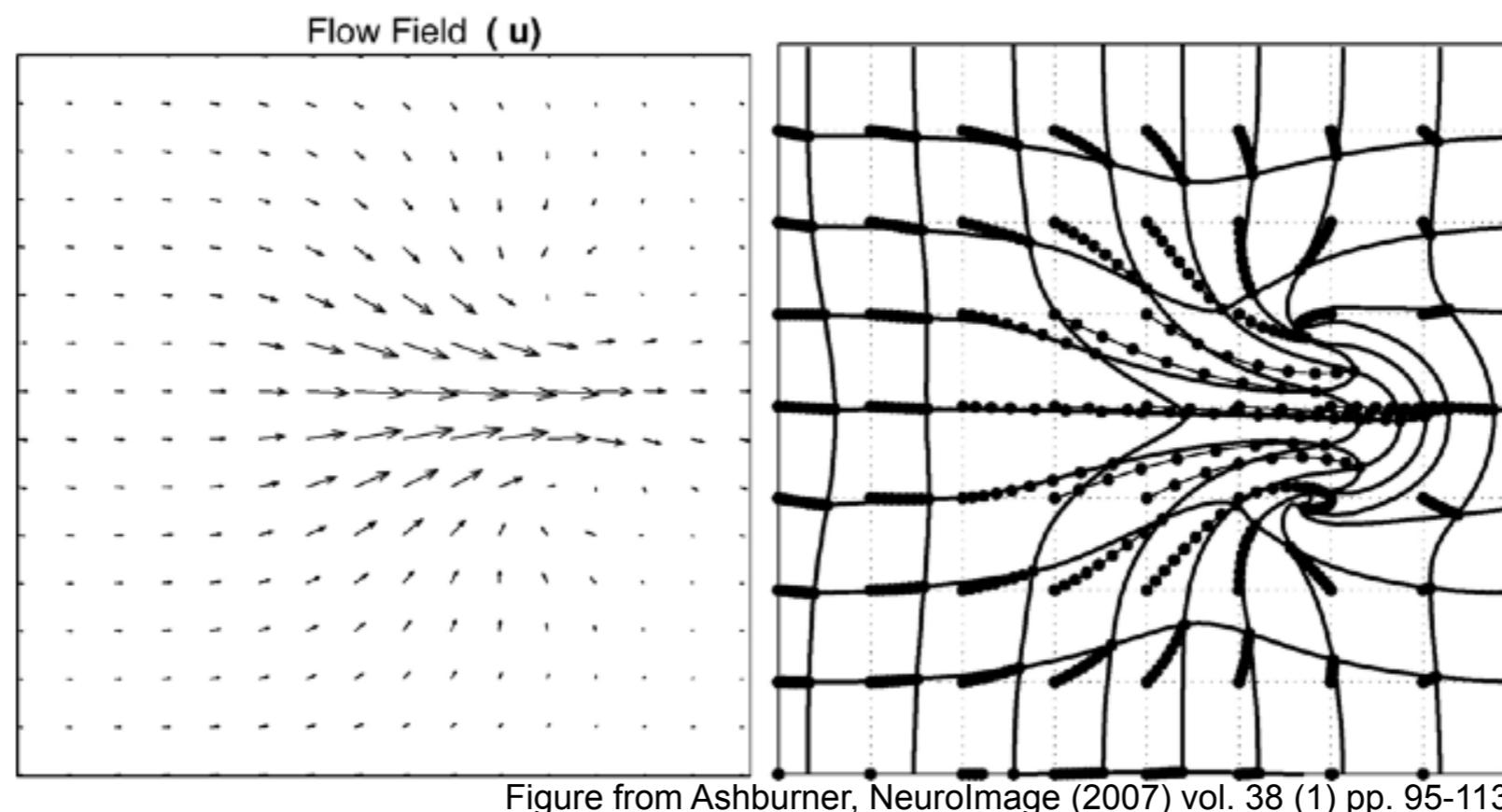
**Theorem 1.** *A FFD based on cubic B-splines is locally injective over all the domain if  $\delta_x < \frac{1}{K}$ ,  $\delta_y < \frac{1}{K}$  and  $\delta_z < \frac{1}{K}$ .*

Choi and Lee [21] have determined a value of  $K \approx 2.48$  so that the maximum displacement of control points given by the bound  $\frac{1}{K}$  is approximately 0.40. This means that the maximum displacement of control points is given by the spacing of control points in the lattice. For example, for a lattice with 20mm control point spacing the maximum control point displacement is 8mm while for a lattice with 2.5mm control point spacing the maximum control point displacement is 1mm.

From Rueckert et al., MICCAI'06

# Velocity field parametrisation

- Integration of a flow field over time to generate a deformation field



$$\exp(\text{Velocity field}) = \text{Deformation Field}$$

# Velocity field parametrisation

- How to integrate a velocity field parametrisation
  - Euler integration
    - Composition of infinitesimally small steps

$$\exp(a + b) = \exp(a) \exp(b)$$

$$\exp(v) = \exp(N \times \frac{v}{N}) = \prod_0^{N-1} \exp(\frac{v}{N})$$

if  $a$  and  $b$  are close to identity:  $\exp(a + b) \approx a \circ b$

$$\exp(v) = \frac{v}{N} \circ \frac{v}{N} \circ \frac{v}{N} \circ \frac{v}{N} \circ \dots, \text{ with } N \gg 1$$

# Velocity field parametrisation

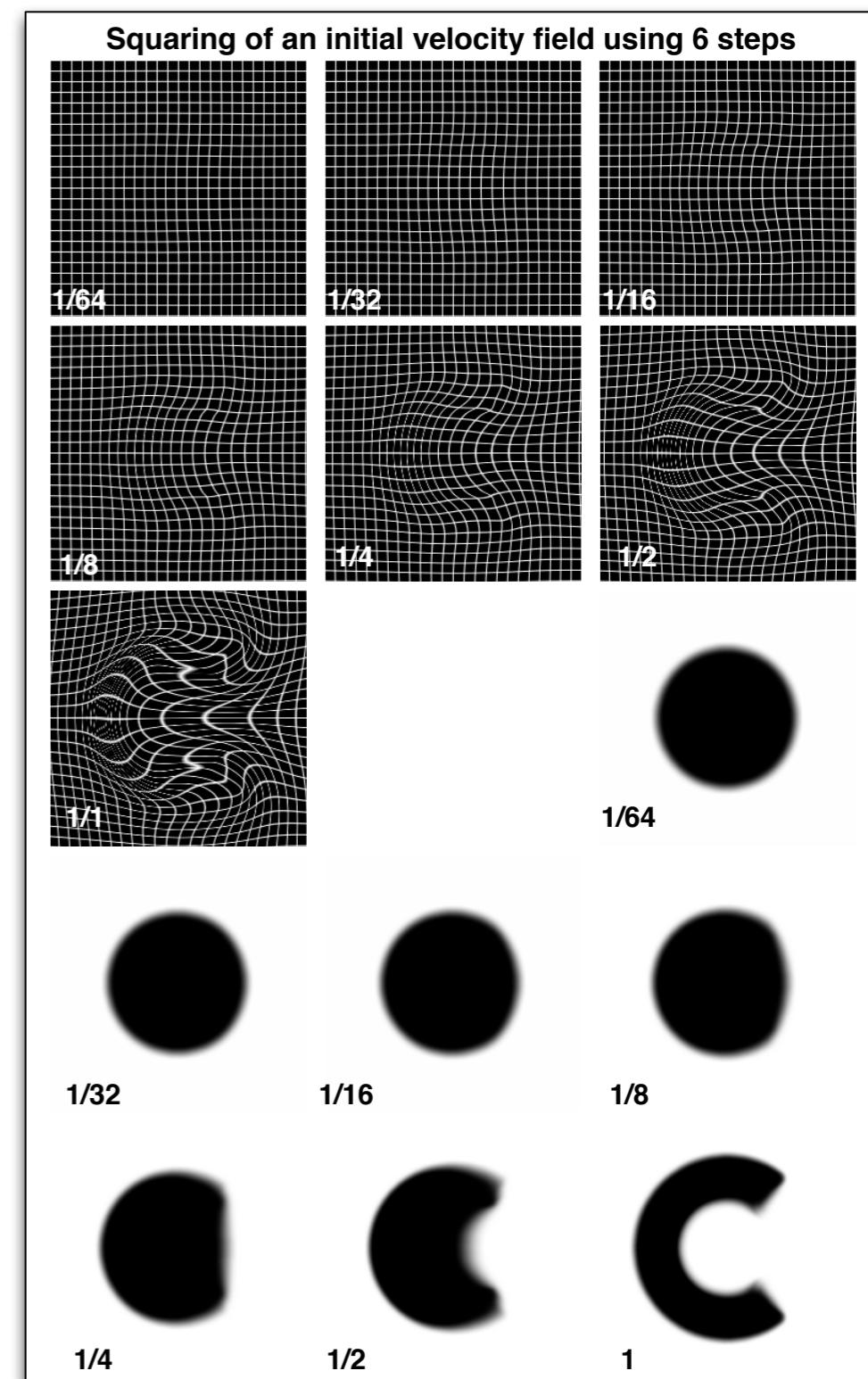
- How to integrate a velocity field parametrisation
  - Euler integration is computationally expensive

$$\begin{aligned}\phi^{1/64} &= x + u(x)/8 \\ \phi^{2/64} &= \phi^{1/64} \circ \phi^{1/64} \\ \phi^{3/64} &= \phi^{1/64} \circ \phi^{2/64} \\ \vdots &= \vdots \\ \phi^{64/64} &= \phi^{1/64} \circ \phi^{63/64}\end{aligned}$$

# Velocity field parametrisation

- How to integrate a velocity field parametrisation
  - Euler integration is computationally expensive
  - Scaling and squaring for stationary velocity field

$$\begin{aligned}
 \phi^{1/64} &= x + u(x)/64 \\
 \phi^{2/64} &= \phi^{1/64} \circ \phi^{1/64} \\
 \phi^{4/64} &= \phi^{2/64} \circ \phi^{2/64} \\
 \phi^{8/64} &= \phi^{4/64} \circ \phi^{4/64} \\
 \phi^{16/64} &= \phi^{8/64} \circ \phi^{8/64} \\
 \phi^{32/64} &= \phi^{16/64} \circ \phi^{16/64} \\
 \phi^{64/64} &= \phi^{32/64} \circ \phi^{32/64}
 \end{aligned}$$



# DARTEL

## Diffeomorphic Anatomical Registration Through Exponential Lie algebra

- Takes advantage of the scaling-and-squaring

$$\exp(v) \exp(-v) = 0$$

$$\exp(v) = \exp(-v)^{-1}$$

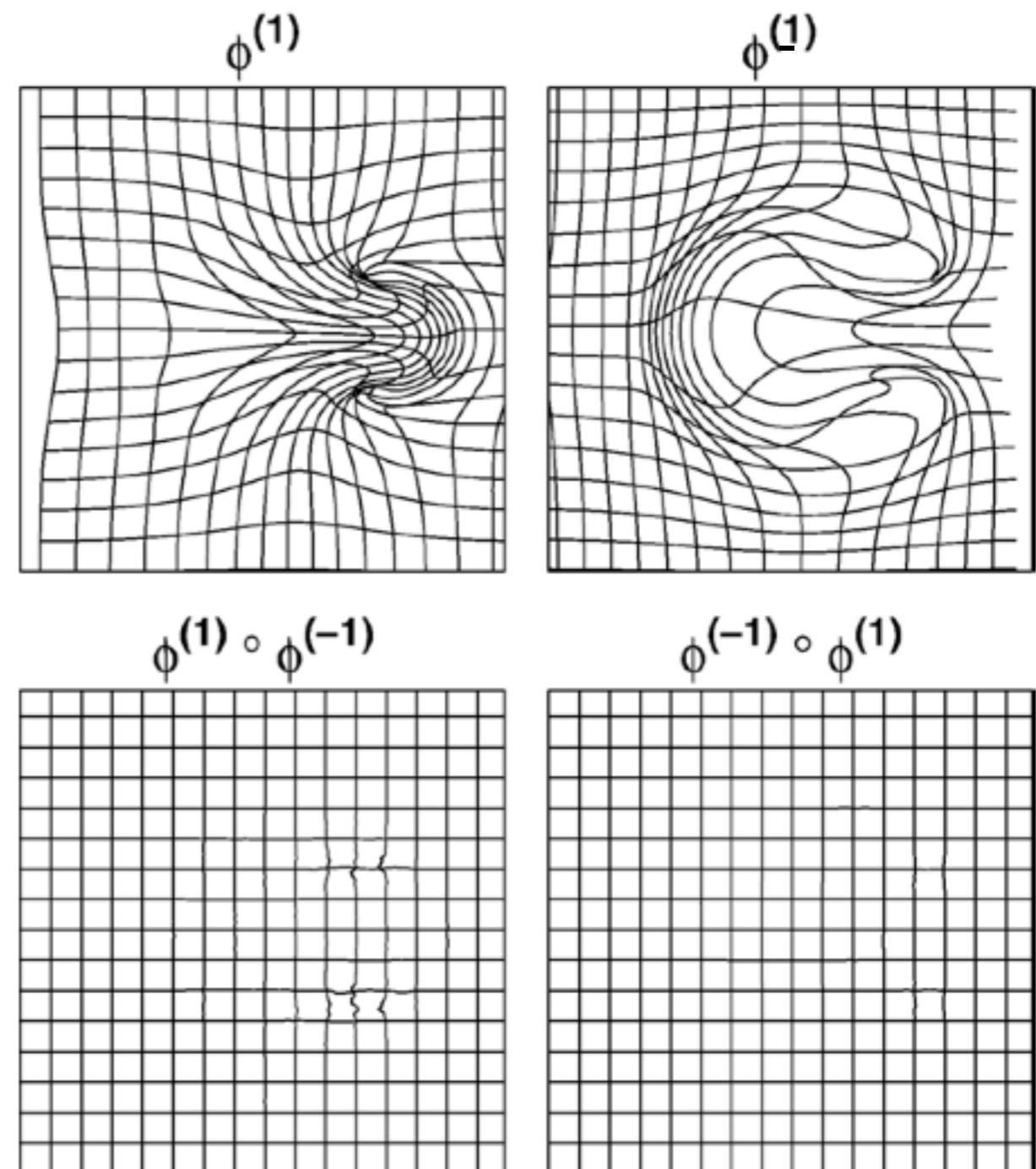


Figure from Ashburner, *NeuroImage*  
(2007) vol. 38 (1) pp. 95-113

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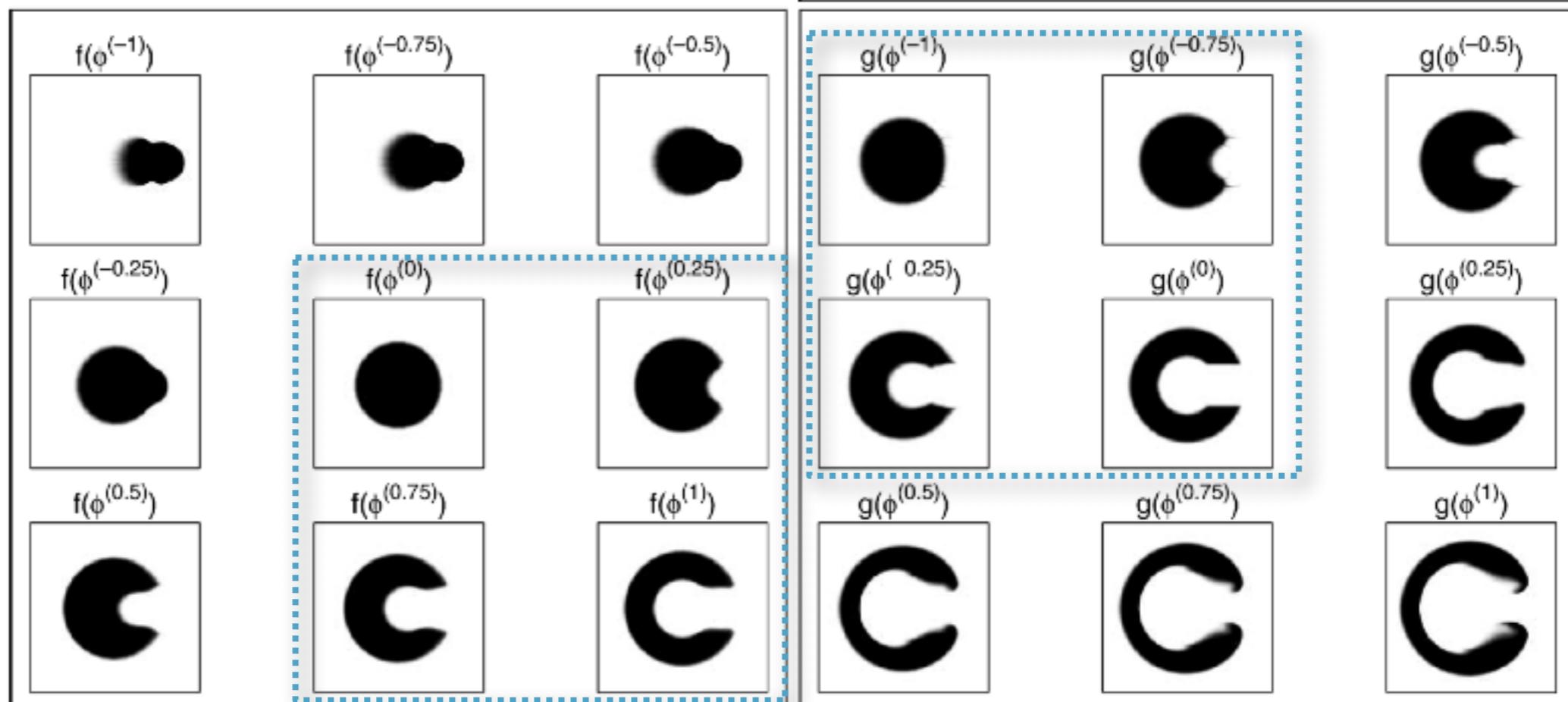
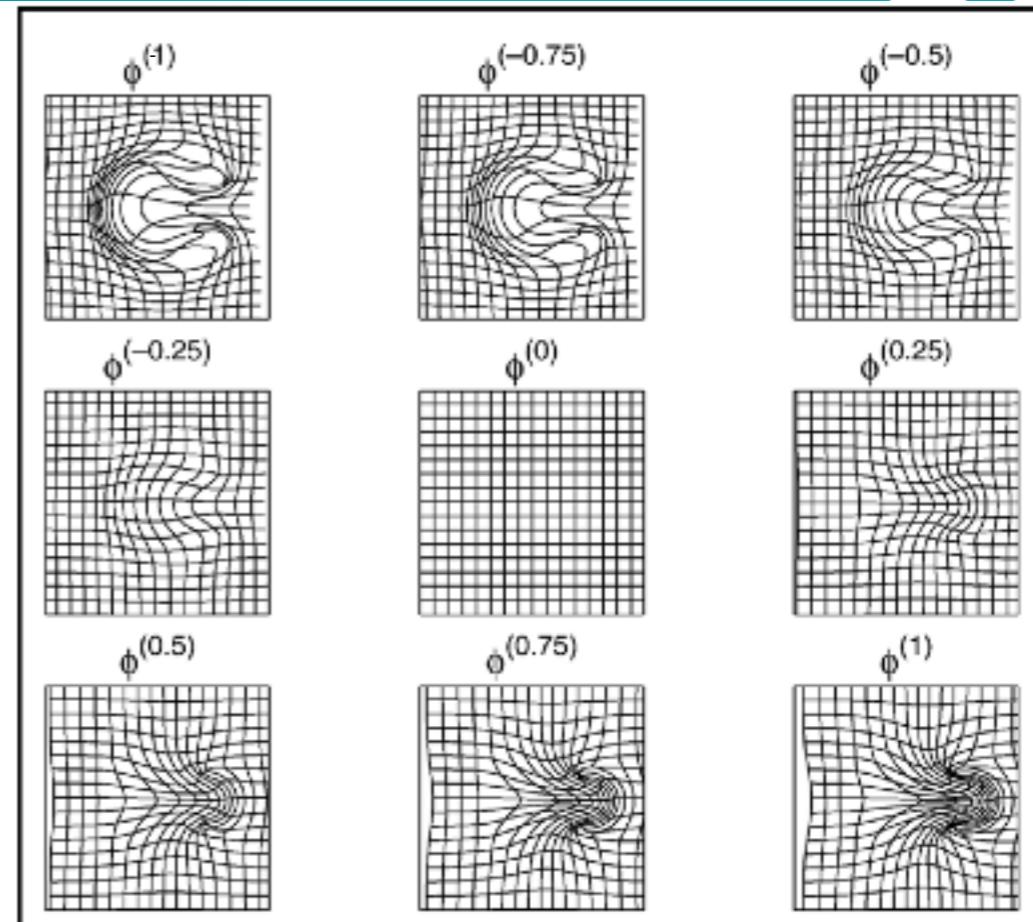
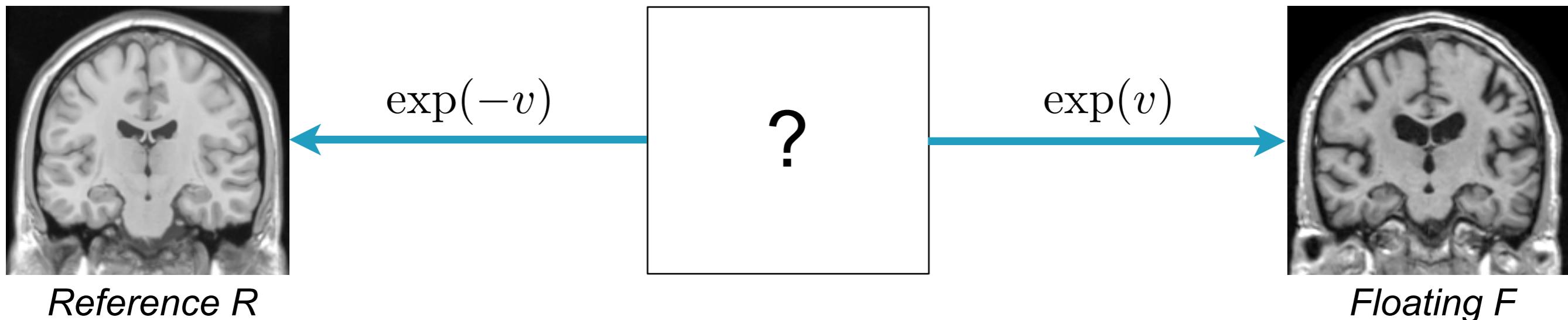


Figure from Ashburner, NeuroImage (2007) vol. 38 (1) pp. 95-113

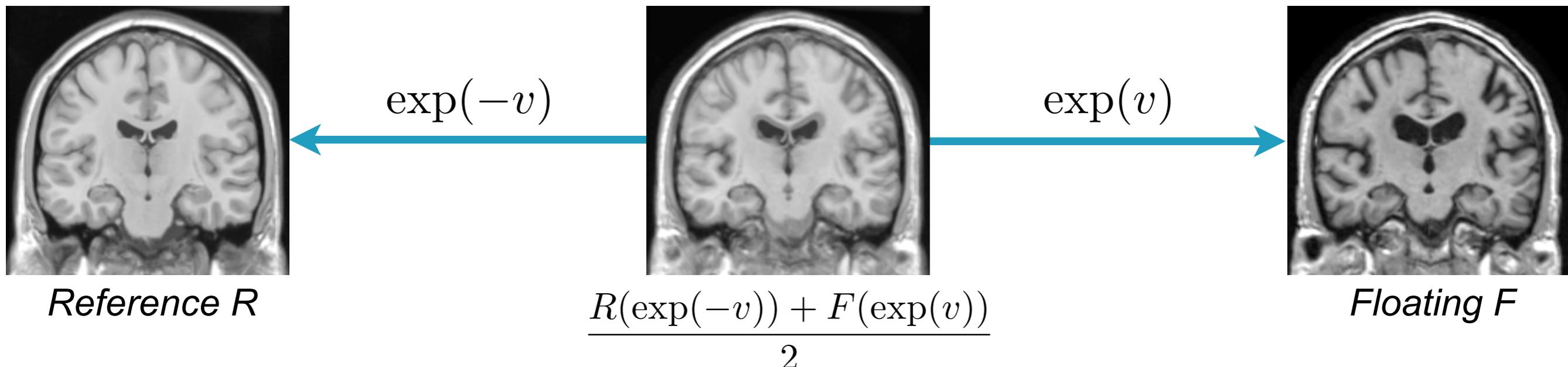
# Symmetric demons

- Use of the stationary velocity field and an average space



# Symmetric demons

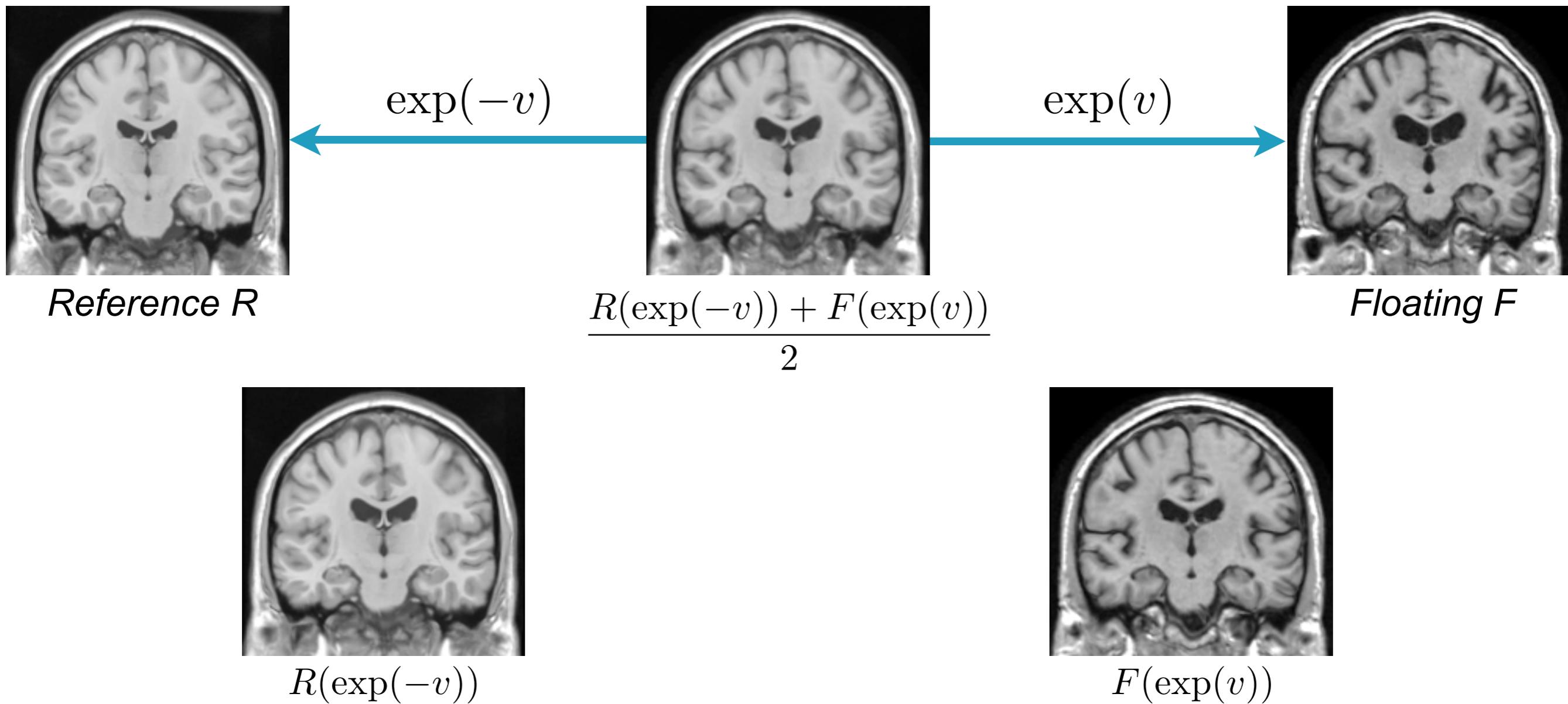
- Use of the stationary velocity field and an average space



Starting with:  $\exp(v) = \exp(-v) = \text{Identity}$

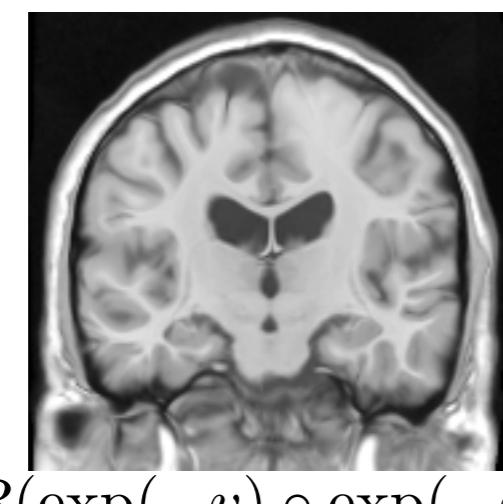
# Symmetric demons

- Use of the stationary velocity field and an average space

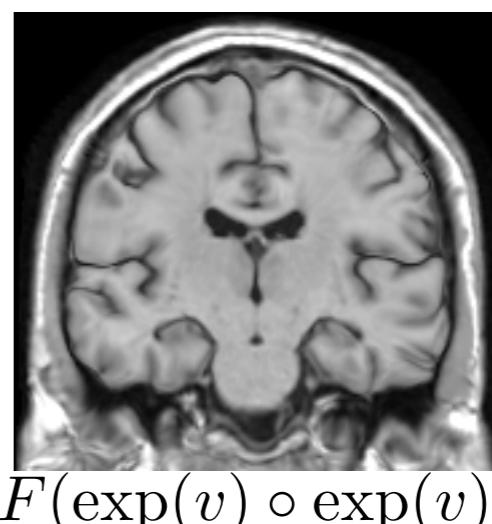


# Symmetric demons

- Use of the stationary velocity field and an average space



$R(\exp(-v) \circ \exp(-v))$



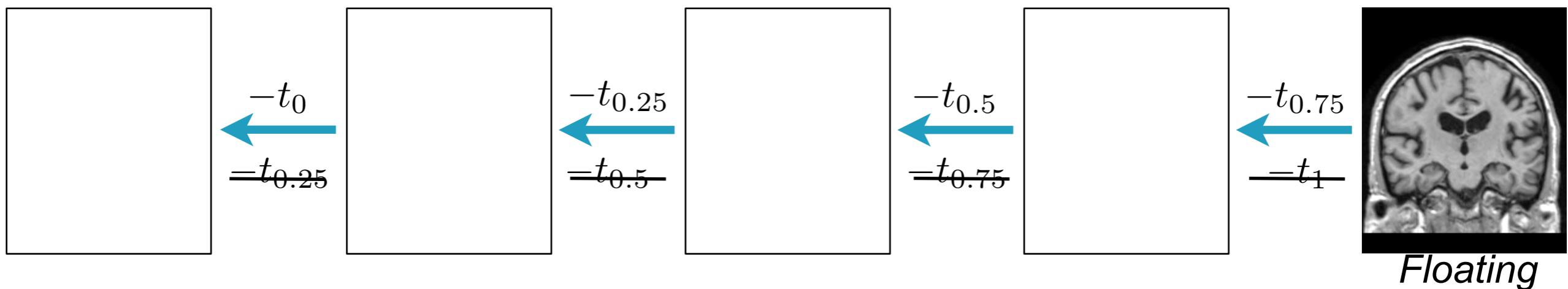
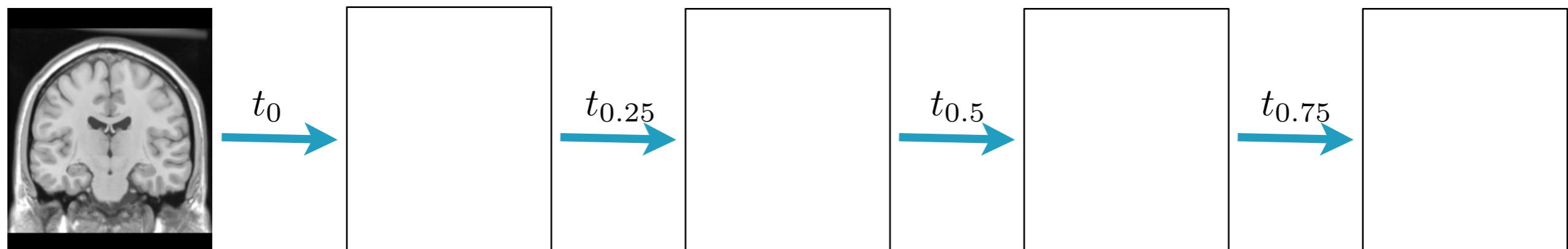
$F(\exp(v) \circ \exp(v))$

# LDDMM

**Large Deformations Diffeomorphic Metric Mapping**

- Non-stationary velocity field optimisation (time-varying)
- Optimisation of geodesics

*Reference*

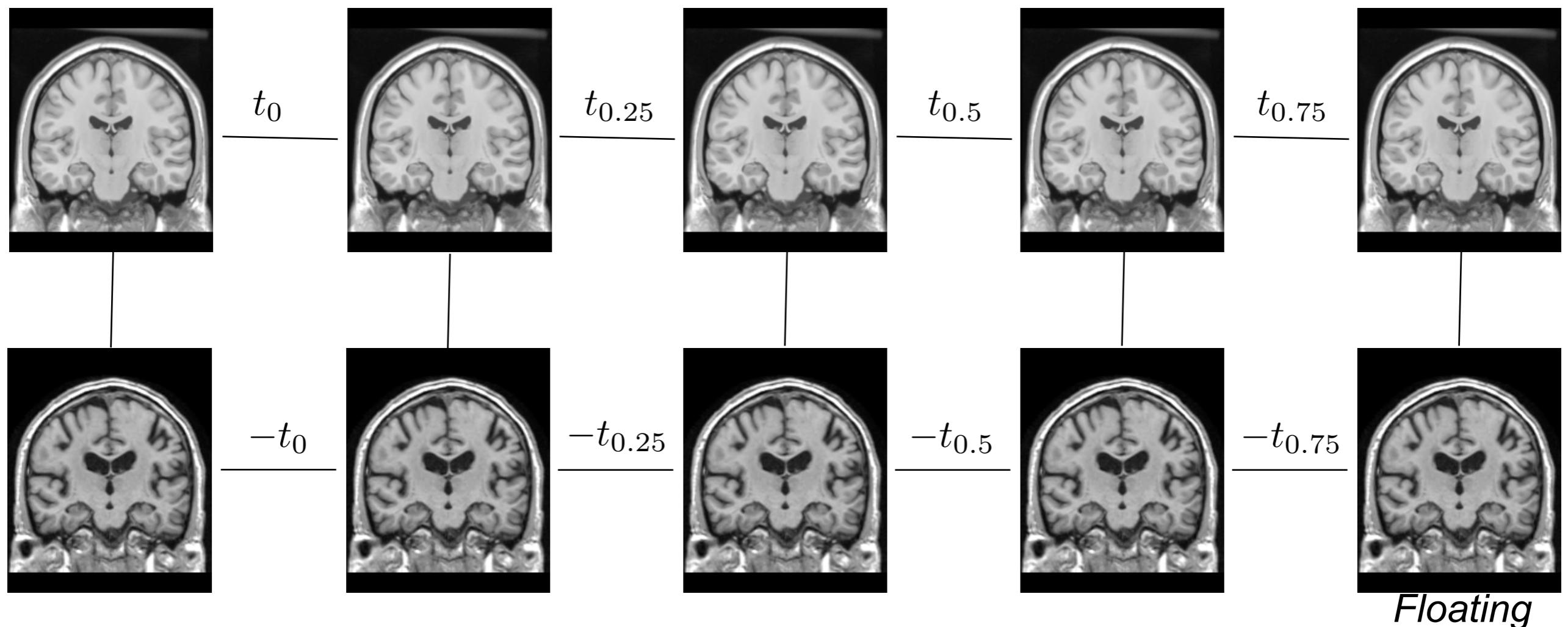


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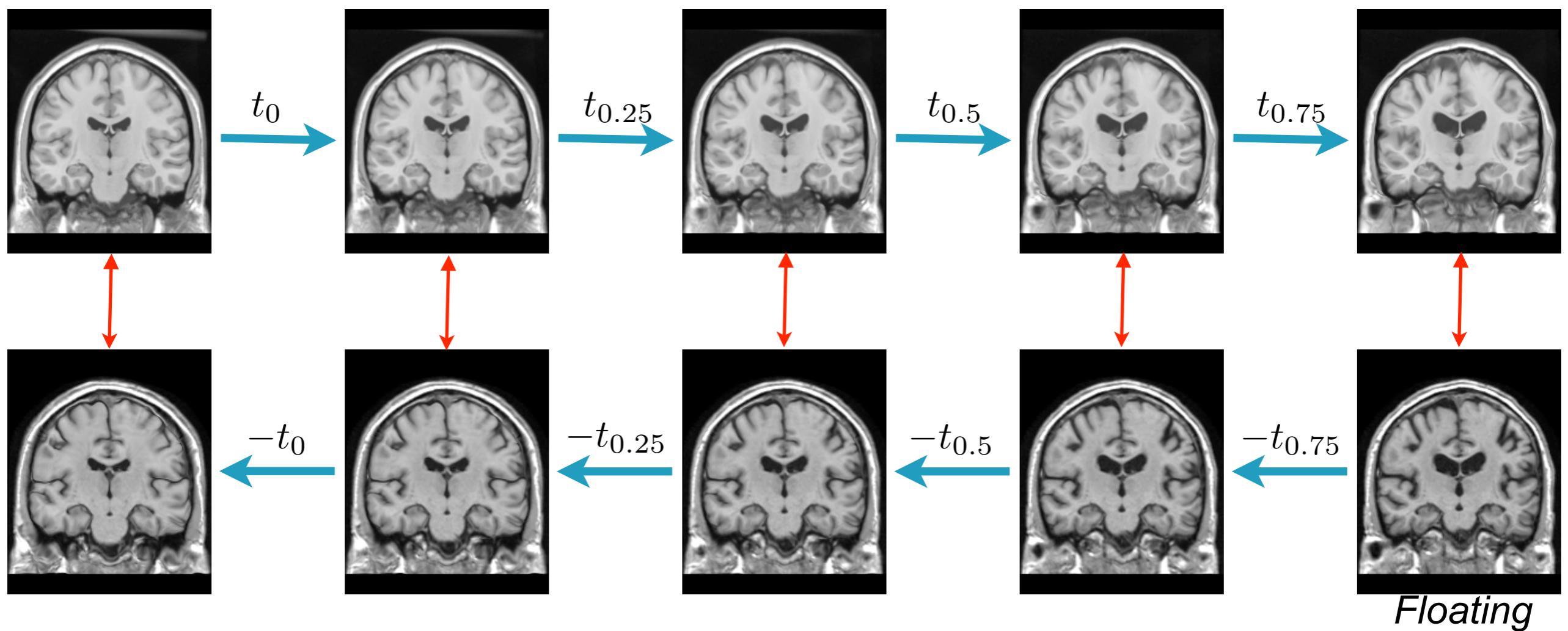


# LDDMM

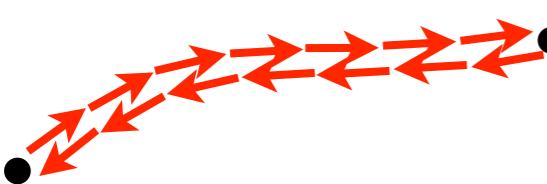
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- Optimisation of geodesics

*Reference*



# Comparison

	Advantages	Drawbacks
Soft or hard constraints on the transformation	 <p>Simple optimisation as additive scheme can be used</p>	<p>Asymmetric transformation model</p> <p>Transformation paths are lost</p>
Stationary velocity field	 <p>Optimisation of forward and backward direction</p> <p>Possibility to average transformations (groupwise)</p>	<p>More complicated optimisation as additive scheme cannot be used anymore</p>
Non-stationary velocity field	 <p>Optimisation of geodesics (Useful to compute distances between images)</p>	<p>Computationally very expensive</p>

# Medical image registration

- Overall scheme

