

¹ GIRFReco.jl: An Open-Source Pipeline for Spiral Magnetic Resonance Image (MRI) Reconstruction in ² Julia ³

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Summary

¹¹ Magnetic Resonance Imaging (MRI) acquires data in the frequency domain (k-space), with
¹² the sampling pattern traversed by a path known as the k-space trajectory. It is desirable
¹³ to implement MRI data sampling using k-space trajectories with high acquisition efficiency
¹⁴ (i.e., a fast coverage of k-space). Traditional Cartesian MRI traverses k-space by acquiring
¹⁵ individual lines of the k-space, each requiring an excitation, a phase-encoding step, and a
¹⁶ short readout gradient. However, it is possible to traverse k-space with an arbitrary trajectory,
¹⁷ achieved by a long sequence of readout gradients, thus presenting the opportunity to acquire
¹⁸ more sampling points per excitation. Spiral trajectories are a popular and efficient method
¹⁹ for traversing k-space with a long readout, as well as classical echo-planar imaging (EPI)
²⁰ trajectories. Non-Cartesian trajectories, such as spiral trajectories, yield significant reductions
²¹ in the number of excitations required for the acquisition of an image, thus offering considerable
²² acceleration and improvements in signal-to-noise ratio (SNR) per unit time at the cost of
²³ reconstruction complexity. These improvements are particularly beneficial in diffusion MRI due
²⁴ to sequence timing constraints (Lee et al., 2021).

²⁵ The actual k-space trajectory applied during the MRI experiment can differ from the nominal
²⁶ trajectory due to hardware imperfections, resulting in image artifacts such as ghosting, blurring
²⁷ or geometric distortion. This problem is exacerbated in many non-Cartesian trajectories, such
²⁸ as spirals, because these fast imaging protocols place high demands on the gradient hardware
²⁹ of the MRI system (Block & Frahm, 2005). Accurate characterization of the system hardware
³⁰ is necessary and can be used for k-space trajectory correction, for example via a gradient
³¹ impulse response function (GIRF) (Addy et al., 2012; Vannesjo et al., 2013).

³² The high acquisition efficiency of non-Cartesian trajectories originates, in part, from the prolonged
³³ readout duration which allows for more samples to be acquired per excitation
³⁴ (single-shot or few-interleave scanning). However, when using such long readouts, the image
³⁵ encoding scheme is susceptible to static off-resonance (or field inhomogeneity, B_0), resulting
³⁶ in image artifacts that scale with readout duration. For non-Cartesian trajectories, these
³⁷ artifacts are difficult to correct in post-processing, but can be effectively addressed during
³⁸ image reconstruction by incorporating spatial off-resonance measurements into the signal model
³⁹ (Sutton et al., 2003).

⁴⁰ Therefore, recent spiral imaging approaches often rely on an expanded signal model incorporating
⁴¹ system imperfections and off-resonance maps (Engel et al., 2018; Graedel et al., 2021; Kasper
⁴² et al., 2018; Kasper et al., 2022; Lee et al., 2021; Robison et al., 2019; Vannesjo et al., 2016;

43 Wilm et al., 2011, 2015), in combination with parallel imaging acceleration using multiple
44 receiver coils and iterative non-Cartesian image reconstruction algorithms, e.g., CG-SENSE
45 (Pruessmann et al., 2001).

46 Here, we introduce the open-source GIRFReco.jl reconstruction pipeline, which provides a
47 single ecosystem implementation of this state-of-the-art approach to non-Cartesian MRI in the
48 programming language Julia (Bezanson et al., 2017). The core reconstruction routines rely
49 upon the public Julia package MRIReco.jl, a comprehensive open-source image reconstruction
50 toolbox. To enable robust, accessible and fast MRI with spiral gradient waveforms, GIRFReco.jl
51 is designed as an end-to-end signal processing pipeline, from open-standard raw MR data
52 ([ISMR]MRD (Inati et al., 2017)) to final reconstructed images (NIfTI neuroimage data format
53 (NIFTI, 2003)). It integrates system characterization information via GIRF correction for
54 accurate representation of the encoding fields, relevant calibration data (coil sensitivity and
55 static off-resonance maps) and iterative parallel imaging reconstruction for non-Cartesian
56 k-space sampling patterns, including spiral trajectories.

57 Statement of Need

58 Existing open-source solutions for the correction of system imperfections and static off-resonance
59 in MRI are often implemented within the framework of mature image reconstruction suites
60 such as BART (Blumenthal et al., 2022), Gadgetron (Hansen & Sørensen, 2013) and MIRT
61 (Fessler, n.d.).

62 However, the aforementioned complexity of the image reconstruction task for spiral MRI
63 currently necessitates the integration of tools from multiple of these software suites in order to
64 establish a performant and comprehensive image reconstruction workflow (e.g., (Veldmann et
65 al., 2022)). With each tool being developed in different programming languages (C for BART;
66 C++ for Gadgetron; MATLAB, C++ and C for MIRT, etc.), maintaining and extending such
67 an image reconstruction pipeline then requires cross-language expertise, adding significant
68 overhead and complexity to development. This presents a significant barrier to efficient and
69 reproducible image reconstruction and limits software accessibility and sustainability, especially
70 for users without software engineering backgrounds.

71 The programming language Julia (Bezanson et al., 2017) provides a practical solution to this
72 multiple-language problem by using a high-level interface to low-level compiled code, i.e.,
73 enabling fast prototyping with limited resources in an academic setting, while delivering a
74 near-industrial-level efficiency of code execution, all within a single development environment.

75 In this work, we introduce GIRFReco.jl (initial version presented at the annual meeting
76 of ISMRM 2022 (Jaffray et al., 2022b)), which implements an end-to-end, self-contained
77 processing and image reconstruction pipeline for spiral MR data completely in Julia. Based
78 on the established MRIReco.jl package, GIRFReco.jl incorporates model-based corrections
79 (Sutton et al., 2003; Vennesjo et al., 2016; Wilm et al., 2011, 2015) to achieve high-quality spiral
80 MRI reconstructions. Specifically, this reconstruction pipeline combines several major steps: (1)
81 ESPIRiT coil sensitivity map estimation (Uecker et al., 2014); (2) Robust off-resonance (B_0)
82 map estimation (Funai et al., 2008; Lin & Fessler, 2020); (3) Computation of the applied non-
83 Cartesian k-space trajectory using GIRF correction (Vennesjo et al., 2013, 2016); (4) Iterative
84 non-Cartesian MRI reconstruction (CG-SENSE) with off-resonance correction (Knopp et al.,
85 2009; Pruessmann et al., 2001). Considering software reusability and sustainability, (1) and (4)
86 of the abovementioned steps are handled by MRIReco.jl, a comprehensive modular open-source
87 image reconstruction toolbox in Julia. Step (2), the B_0 map estimation, was developed as
88 a Julia package MRIFieldmaps.jl by the original authors (Lin & Fessler, 2020) with our
89 contribution of implementing an alternative algorithm (Funai et al., 2008) in Julia. Finally,
90 we implemented step (3), the GIRF correction, in an original Julia package MRIGradients.jl
91 (Jaffray et al., 2022b), porting and refactoring the MATLAB code of the original authors
92 (Vennesjo & Graedel, 2020).

93 **Functionality**

94 **Required Inputs**

95 `GIRFReco.jl` requires raw MRI (k-space) data (in [ISMR]MRD format ([Inati et al., 2017](#))) of
96 the following scans as input:

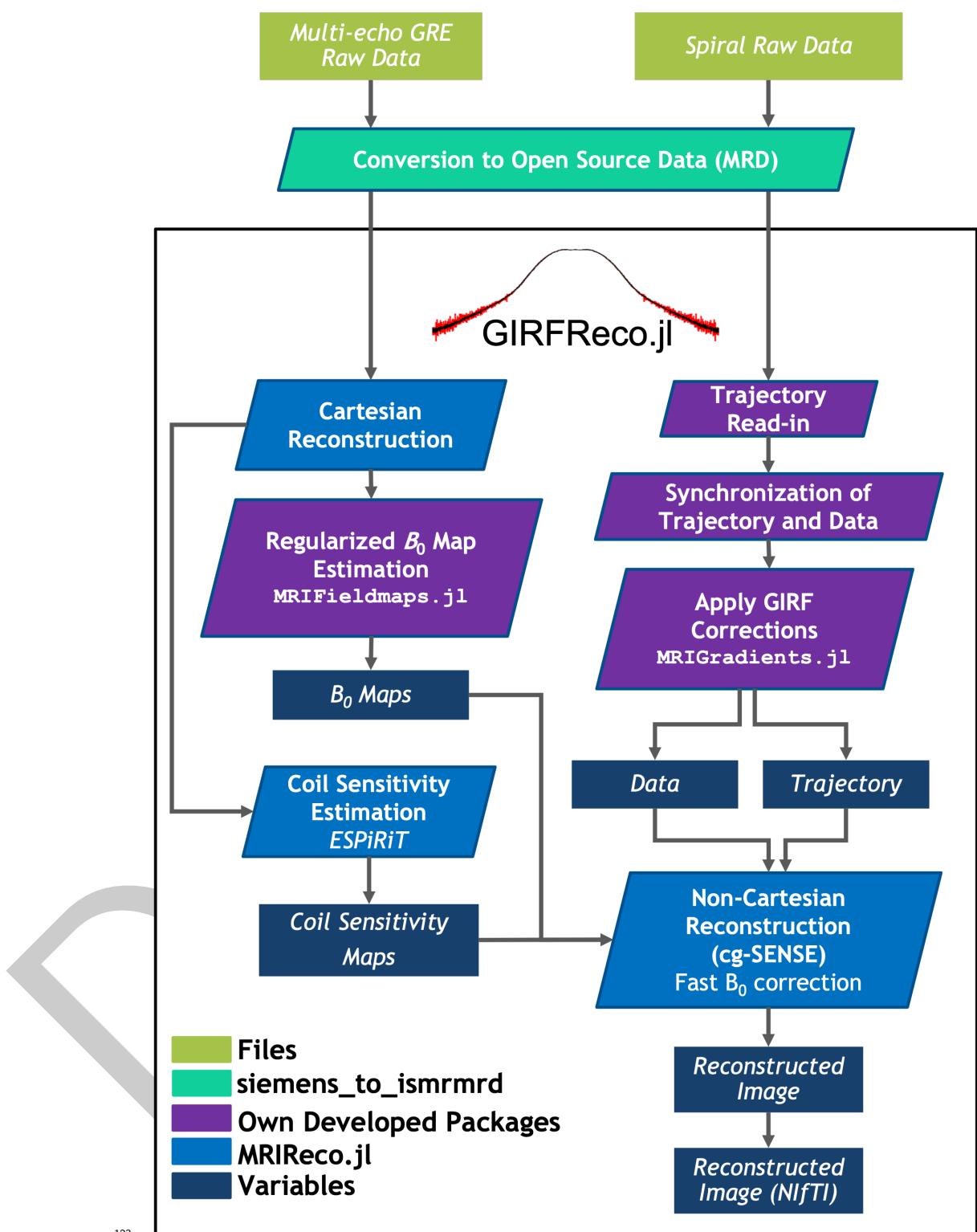
- 97 1. Multi-echo Gradient-echo spin-warp (Cartesian) scan
 - 98 ▪ must include at least two echo times (e.g., 4.92 ms and 7.38 ms at 3T)
- 99 2. Spiral scan
 - 100 ▪ single or multi-interleave

101 At the moment, the slice geometry (thickness, field-of-view, and direction) of the Cartesian and
102 spiral scans must be congruent, while the resolution does not need to be identical or isotropic.

103 **Overview of Components**

104 The following components are utilized within the spiral reconstruction pipeline of `GIRFReco.jl`
105 (Fig. 1), and called from their respective packages. We indicate where the authors of
106 `GIRFReco.jl` provided original contributions to the components by bold font.

- 107 1. Core iterative image reconstruction, using the Julia package `MRIReco.jl`
 - 108 a. CG-SENSE ([Pruessmann et al., 2001](#)) algorithm for iterative non-Cartesian image
109 reconstruction
 - 110 b. ESPIRiT ([Uecker et al., 2014](#)) for sensitivity map estimation
- 111 2. Model-based correction
 - 112 a. Static off-resonance (B_0 inhomogeneity) correction
 - 113 ▪ **Smoothed B_0 map estimation, using an implementation of** ([Funai et al., 2008](#)) and `MRIFieldMaps.jl` ([Lin & Fessler, 2020](#))
 - 114 ▪ Static B_0 map correction, accelerated by a time-segmented implementation
115 ([Knopp et al., 2009](#)) in `MRIReco.jl` ([Knopp & Grosser, 2021](#))
 - 116 b. Encoding field (trajectory) correction via Gradient impulse response function (GIRF)
117 ([Vannesjo et al., 2013](#))
 - 118 ▪ Measurement with a phantom-based technique ([Addy et al., 2012; Graedel et
119 al., 2017; Robison et al., 2019](#))
 - 120 ▪ **Estimation using open-source code** ([Wu et al., 2022](#))
 - 121 ▪ **Prediction via `MRIGradients.jl`** ([Jaffray et al., 2022b](#))



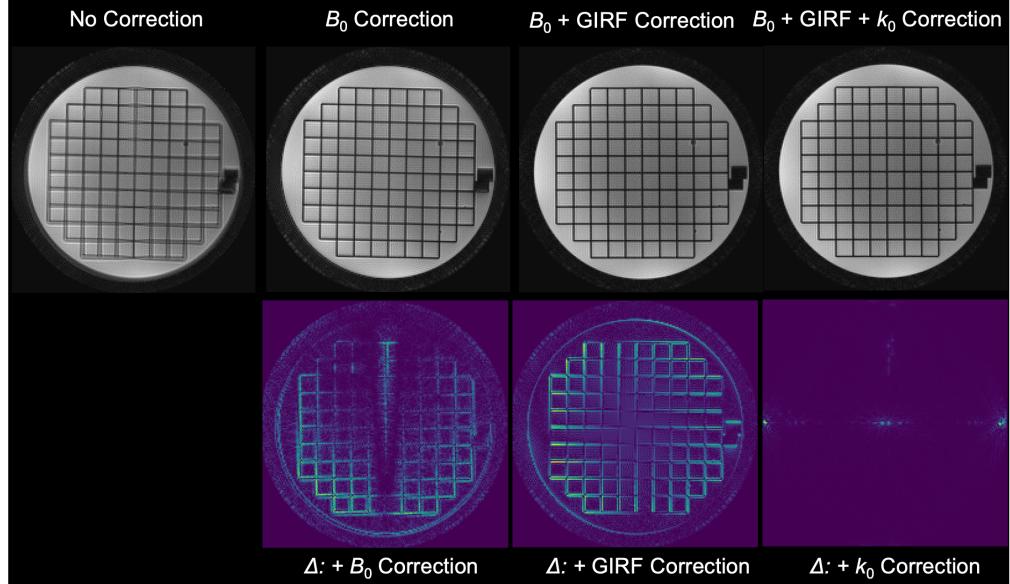
123 *Figure 1.* Overview of the `GIRFReco.jl` signal processing and reconstruction pipeline. Depicted
 124 is the workflow from raw acquired k -space data to the final reconstructed images with the
 125 respective tasks (parallelogram), in/output data (rectangles) and the location of the processing
 126 components within different packages (colours).
 127

128 Detailed Processing Pipeline

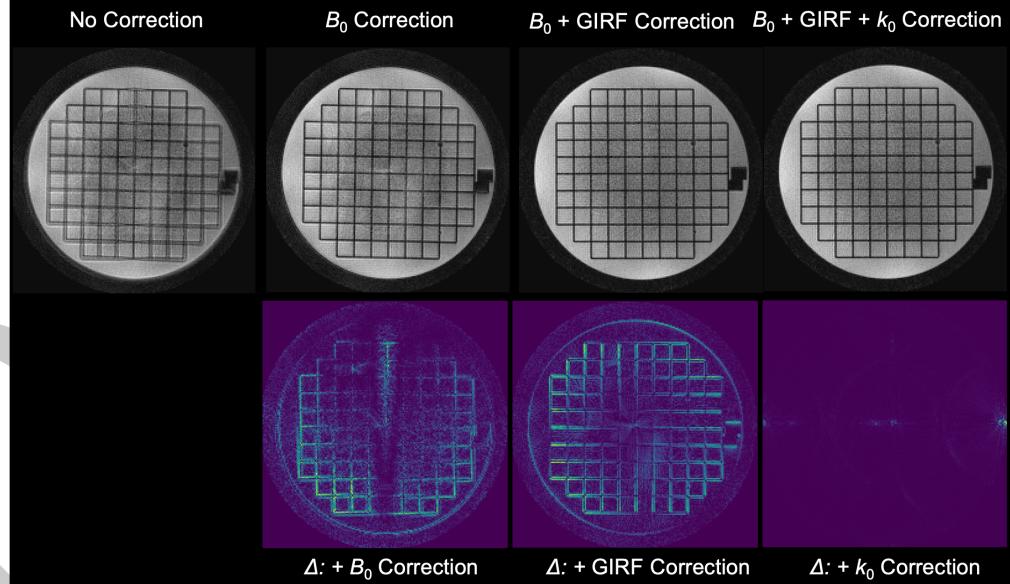
129 GIRFReco.jl executes the steps required (depicted in Figure 1) for spiral diffusion reconstruction
130 in the following order:

- 131 1. Conversion of proprietary, vendor-specific raw image data to an open-source raw data
132 format ([ISMR]MRD, ([Inati et al., 2017](#))).
 - 133 2. Reading of the trajectory or gradient sequence and synchronization of the k-space
134 trajectory onto the time course of the sampled k-space data to resolve any sampling rate
135 differences.
 - 136 3. Model-based correction of the k-space sampling points (linear gradient self-terms) and
137 data (k_0 eddy currents) using the gradient impulse response function (GIRF ([Vannesjo](#)
138 [et al., 2013](#)), MRIGradients.jl ([Jaffray et al., 2022b](#))).
 - 139 4. Iterative reconstruction of Cartesian multi-echo gradient echo (GRE) scan.
 - 140 5. Coil sensitivity map estimation (ESPIRiT ([Uecker et al., 2014](#)), MRIReco.jl) from the
141 first echo of multi-echo Cartesian GRE data.
 - 142 6. Off-resonance (B_0) map estimation and processing (MRIFieldmaps.jl, ([Funai et al.,](#)
143 [2008; Lin & Fessler, 2020](#))) based on multi-echo Cartesian GRE data.
 - 144 7. Non-Cartesian, iterative parallel image reconstruction (cgSENSE) with off-resonance
145 correction (([Knopp et al., 2009](#); [Pruessmann et al., 2001](#)), MRIReco.jl ([Knopp & Grosser,](#)
146 [2021](#))).
- 147 Via dedicated configuration files, individual steps can be selectively applied or skipped during
148 reconstruction, enabling assessment of the impact of different model-based corrections on
149 final image quality. We demonstrate this use case by providing example reconstructions
150 obtained from the GIRFReco.jl pipeline for a T_2 -weighted four-interleave spiral acquisition of
151 a geometric structure phantom by the American College of Radiology (ACR). Reconstructions
152 of both fully sampled and accelerated (using 1 of 4 interleaves, $R = 4$) datasets are depicted in
153 Figure 2. *In vivo* brain images reconstructed from a T_2 -weighted single-interleave ($R=4$) spiral
154 acquisition are presented in Figure 3 ([Kasper et al., 2023](#)). In all cases, improved image quality
155 was obtained by successively increasing the complexity of the applied model-based corrections
156 (nominal trajectory, added B_0 correction, GIRF-correction of gradients, GIRF correction of
157 k_0 eddy currents). The improvements in quality are best seen when looking at high-contrast
158 features of the images such as edges and corners, with subsequent corrections creating sharper
159 edge contrast and reducing blurring of small features.
- 160 Note that the reconstruction results from the phantom experiments (both $R = 1$ and $R = 4$
161 reconstructions in Figure 2) can be fully reproduced using GIRFReco.jl and the corresponding
162 dataset made publicly available ([Jaffray et al., 2022a](#)). For details, see the “Getting Started”
163 section below.

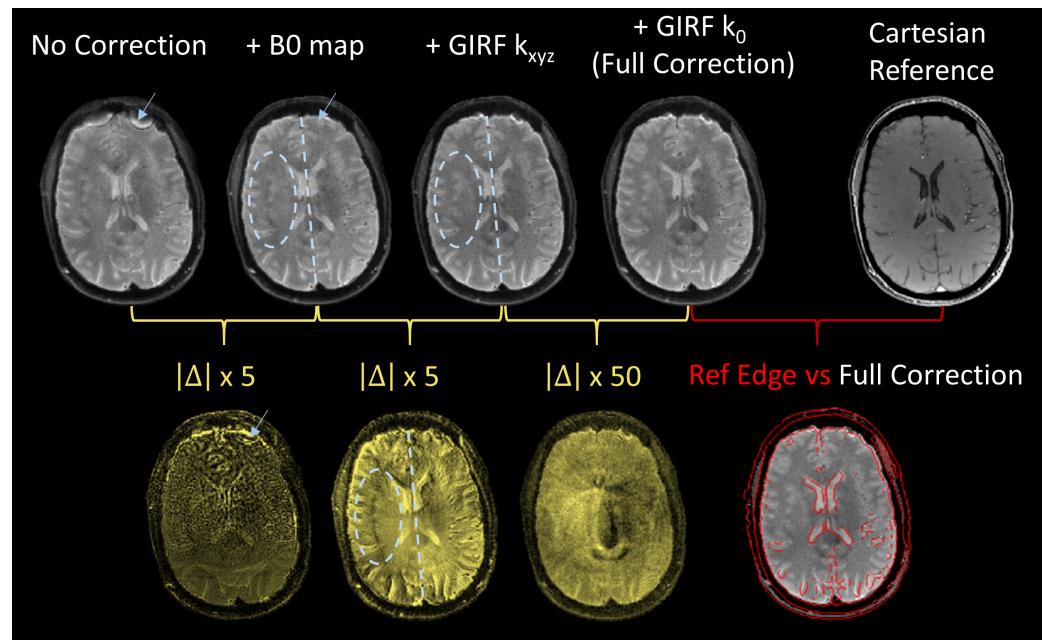
No Acceleration ($R = 1$)



4x Acceleration ($R = 4$)



164
165 *Figure 2.* Reconstructed four-interleave ($R=1$) and single-interleave ($R=4$) spiral images of a
166 selected slice of the ACR phantom. Top row, from left to right: Images reconstructed from the
167 nominal spiral gradient waveforms (“No Correction”), with correction for static off-resonance
168 (“ B_0 Correction”), $B_0 + \text{GIRF}$ correction of the k -space trajectory (“ $B_0 + \text{GIRF}$ Correction”),
169 and additional correction for GIRF k_0 eddy currents (“ $B_0 + \text{GIRF} + k_0$ Correction”). Bottom
170 row: Stepwise difference images between subsequent corrections.



171
172 *Figure 3.* Reconstructed *in-vivo* spiral images of a human brain images (single interleave,
173 undersampling factor $R=4$). Top row: Images reconstructed from the nominal spiral gradient
174 waveform (“No correction”), with correction for static off-resonance (“ B_0 map”), $B_0 +$ GIRF
175 correction of the k -space trajectory (“GIRF k_{xyz} ”), and additional correction for GIRF k_0 eddy
176 currents (“Full Correction”). Bottom row: Consecutive absolute difference images of top-row
177 reconstructions (5x scaled, i.e., $\pm 20\%$ max image intensity; or 50x scaled, i.e., $\pm 2\%$
178 max image intensity). A Cartesian image (echo 1 from the B_0 map scan) is used as the
179 reference; its edges are overlaid to assess geometric congruency of the spiral images.

180 Quality of Life Features

181 In addition to providing an end-to-end reconstruction workflow, GIRFReco.jl offers methods
182 for plotting images and calibration data at intermediate steps throughout the pipeline using
183 PlotlyJS. Furthermore, intermediate reconstruction results, such as calculated coil sensitivity
184 maps and B_0 maps are optionally stored as NIfTI files, a common neuroimaging data format
185 supported by various analysis and visualization packages ([NIfTI, 2003](#)).

186 Getting Started

187 Up-to-date information about how to install GIRFReco.jl, run example reconstructions (e.g.,
188 reproducing Figure 2) and apply it to your own data can be found in the [README.md](#) provided in
189 the GitHub repository. Further example scripts and technical documentation of GIRFReco.jl’s
190 API, including its current feature set, is provided at '<https://brain-to.github.io/GIRFReco.jl>',
191 automatically generated by [Documenter.jl](#).

192 Conclusion and Outlook

193 The presented pipeline, GIRFReco.jl, is an open-source end-to-end solution for spiral MRI
194 reconstruction. It is developed in Julia, and allows users to obtain final images directly from
195 raw MR data acquired by spiral k -space trajectories. Following best practices of software
196 sustainability and accessibility, we rely on the established MR image reconstruction package
197 MRIReco.jl in our pipeline, while extending its capability to handle the more complex use
198 case of multiple model-based corrections, necessary for high-quality spiral MRI. Beyond spirals,

199 GIRFReco.jl can be readily utilized for data acquired under arbitrary non-Cartesian k-space
 200 trajectories; its features of model-based MRI reconstruction with GIRF and off-resonance
 201 corrections generalize to such sampling patterns in both 2D and 3D. Furthermore, GIRFReco.jl
 202 can be extended to handle additional model-based corrections (e.g., concomitant or higher-order
 203 encoding fields, (Bernstein et al., 1998; Vannesjo et al., 2016; Wilm et al., 2011, 2015)),
 204 and act as a self-contained template for generalized image reconstruction from raw scan and
 205 calibration data to interpretable and accessible images in Julia.

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