

Fast Fourier Beamforming for Arbitrary Ultrasound Imaging Sequences Based on a K-Space Implementation of Reverse-Time Migration

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FOURIER BEAMFORMING

- Monostatic Synthetic Aperture¹:
 - Exploding Reflector Model (ERM)
 - $s(t, x)$ vs time t & TX/RX location x
 - $F_{2D}\{s(t, x)\} = S(f, k_x) \rightarrow I(k_x, k_z)$
 - via Stolt mapping $f = \frac{c}{2} \sqrt{k_x^2 + k_z^2}$
- Garcia's Plane-Wave Method²:
 - Modifies ERM parameters to make plane-wave delays agree to 2nd order
- Multistatic Synthetic Aperture^{3,5}:
 - Record signal $s(t, u, v)$ vs time t
 - RX at $x = u$ — TX at $x = v$
 - $F_{2D}\{s(t, u, v)\} = S(f, k_u, k_v) \rightarrow I(k_x, k_z)$
 - $k_x = k_u + k_v$
 - $k_z = \sqrt{\left(\frac{f}{c}\right)^2 - k_u^2} + \sqrt{\left(\frac{f}{c}\right)^2 - k_v^2}$
- Lu's Plane-Wave Method⁴:
 - At angle θ : $k_v = \left(\frac{f}{c}\right) \sin \theta$
 - $k_u = k_x - \left(\frac{f}{c}\right) \sin \theta$
 - $f = \frac{c(k_x^2 + k_z^2)}{2k_z \cos \theta + 2k_x \sin \theta}$
 - $F_{2D}\{s_\theta(t, u)\} = S_\theta(f, k_u) \rightarrow I(k_x, k_z)$

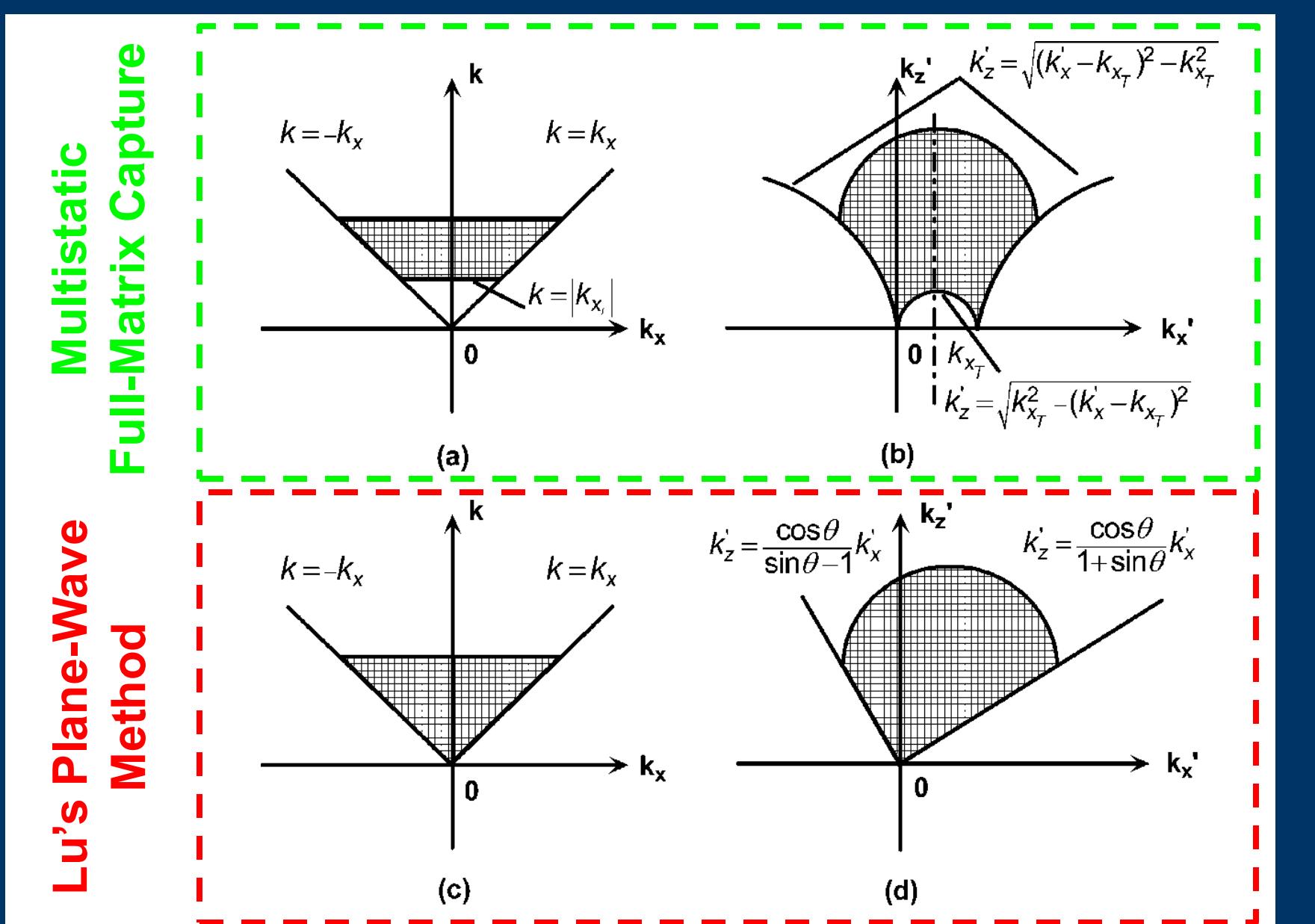


Figure 1. Stolt's mapping in k-space for multistatic synthetic aperture (i.e., full-matrix capture)³ and plane-wave imaging⁴

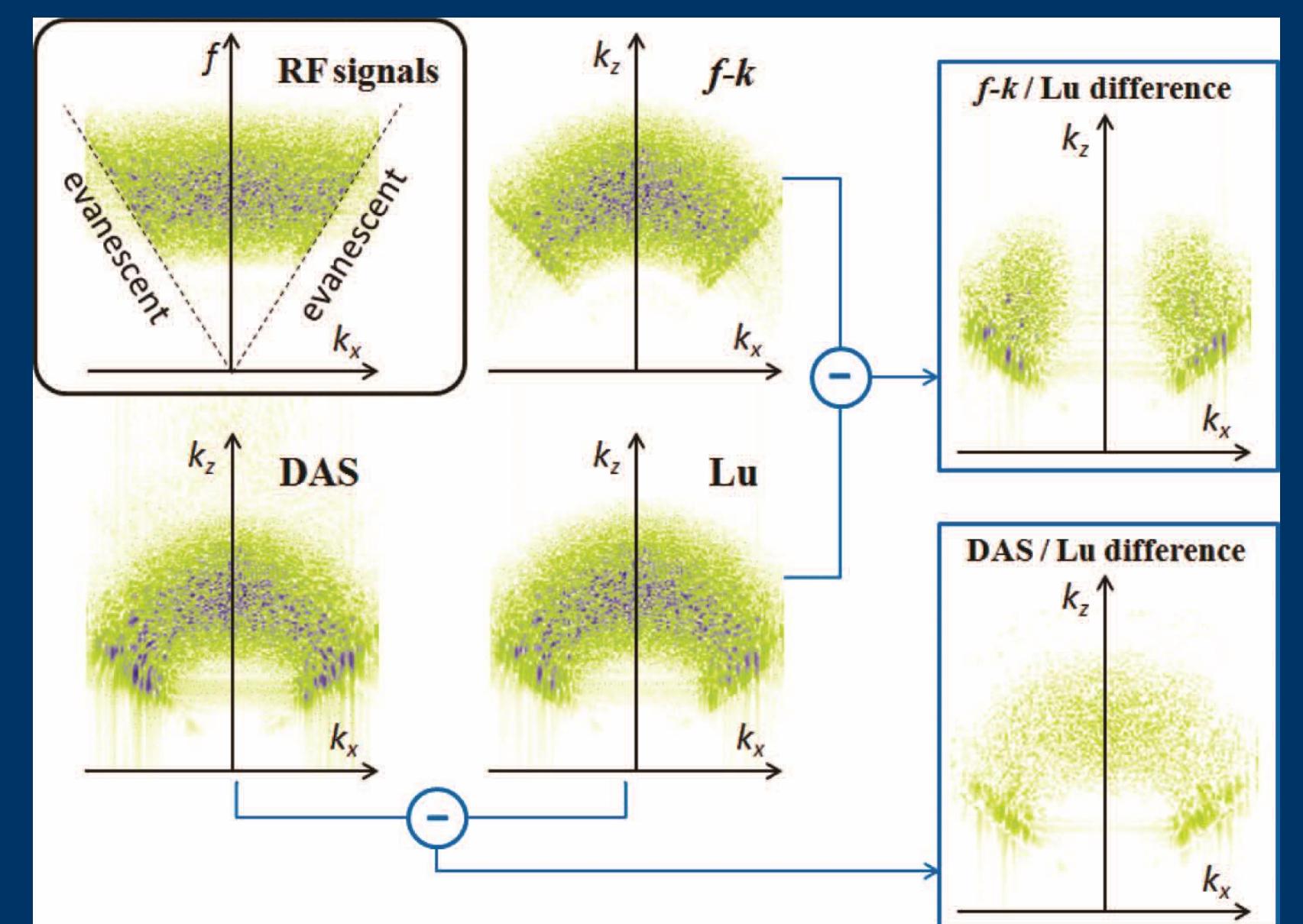


Figure 2. Lu⁴ and Garcia² Fourier Beamformers vs DAS

REVERSE-TIME MIGRATION (RTM)

- TX & RX Wavefields: $p_{tx(i)}(x, z, t)$ and $p_{rx(i)}(x, z, t)$
 - Calculated using Angular Spectrum Method
- Correlation of TX & RX Wavefields (Figure 3):

$$I_i(x, z) = \int_0^\infty p_{tx(i)}^*(x, z, t) p_{rx(i)}(x, z, t) dt$$

$$I_i(x, z) = \int_0^\infty p_{tx(i)}^*(x, z, f) p_{rx(i)}(x, z, f) df$$
- B-Mode Image: $I_{BM}(x, z) = 20 \log_{10} |\sum_{i=1}^{N_{tx}} I_i(x, z)|$

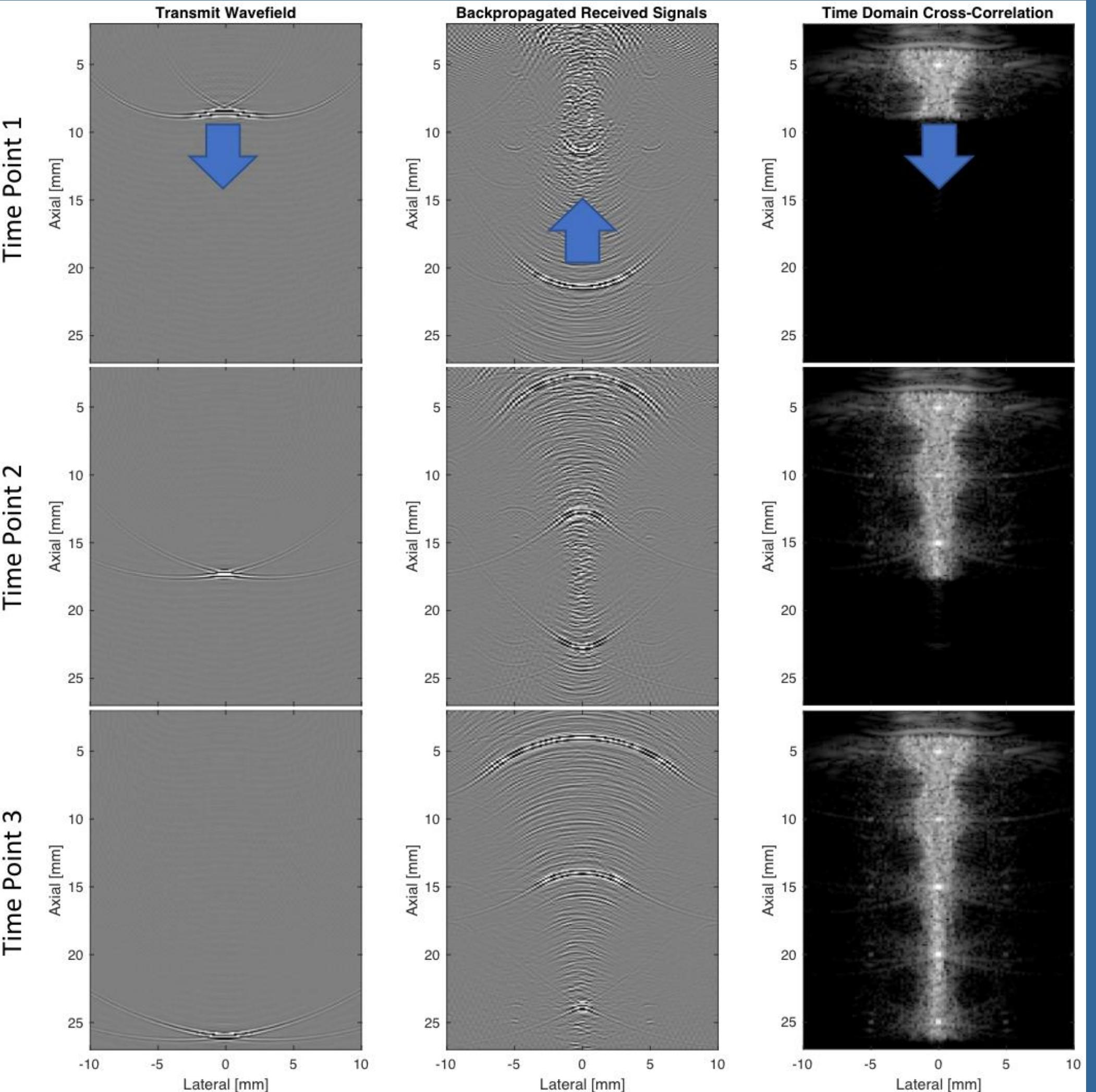


Figure 3. Reverse-Time Migration by Time-Domain Correlation of Transmit Beam Wavefield and Backpropagated Receive Wavefield⁷

ANGULAR SPECTRUM METHOD

- Downward propagation (in z) of TX wavefield:
 - $p_{tx(i)}(k_x, z, f) = \hat{p}_{tx(i)}(k_x, f) e^{-j2\pi(k^2 - k_x^2)^{1/2} z}$
 - $\hat{p}_{tx(i)}(k_x, f) := p_{tx(i)}(k_x, z = 0, f)$
 - $\hat{p}_{tx(i)}(x, f) = A_i(x) P(f) e^{-j2\pi f \tau_i(x)}$
 - Before taking FFT in lateral dimension x
 - TX pulse spectrum $P(f)$
 - TX focal delays $\tau_i(x)$
 - TX apodization $A_i(x)$
- Downward propagation (in z) of RX wavefield:
 - $p_{rx(i)}(k_x, z, f) = \hat{p}_{rx(i)}(k_x, f) e^{+j2\pi(k^2 - k_x^2)^{1/2} z}$
 - $\hat{p}_{rx(i)}(k_x, f) := p_{rx(i)}(k_x, z = 0, f)$
 - Raw RX channel data $\hat{p}_{rx(i)}(x, t)$
 - FFT across lateral dimension x and time t

K-SPACE REPRESENTATION OF RTM

- Inverse Fourier transforms (on TX/RX):

$$p_{tx(i)}(x, z, f) = \int_{-\infty}^{\infty} p_{tx(i)}(k_x^tx, z, f) e^{+j2\pi k_x^tx} dk_x^tx$$

$$p_{rx(i)}(x, z, f) = \int_{-\infty}^{\infty} p_{rx(i)}(k_x^rx, z, f) e^{+j2\pi k_x^rx} dk_x^rx$$
- Body of integral for frequency-domain RTM:

$$p_{tx(i)}^*(x, z, f) p_{rx(i)}(x, z, f) = \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} p_{tx(i)}^*(k_x^tx, z, f) p_{rx(i)}(k_x^rx, z, f) e^{+j2\pi(k_x^rx - k_x^tx)x} dk_x^rx dk_x^tx$$
- If we substitute $k_x^rx = k_x^tx + k_x$:

$$p_{tx(i)}^*(x, z, f) p_{rx(i)}(x, z, f) = \int_{-\infty}^{\infty} C_i(k_x, z, f) e^{+j2\pi k_x x} dk_x$$

$$C_i(k_x, z, f) = \int_{-\infty}^{\infty} p_{tx(i)}^*(k_x^tx, z, f) p_{rx(i)}(k_x^tx + k_x, z, f) dk_x^tx$$
- Insert relations from the angular spectrum method:

$$C_i(k_x, z, f) = \int_{-\infty}^{\infty} \hat{p}_{tx(i)}(k_x^tx, f) \hat{p}_{rx(i)}(k_x^tx + k_x, f) H(k_x, z, k_x^tx, f) dk_x^tx$$

$$H(k_x, z, k_x^tx, f) = e^{+j2\pi[(k^2 - (k_x^tx)^2)^{1/2} + (k^2 - (k_x^tx + k_x)^2)^{1/2}]z}$$

$$H(k_x, z, k_x^tx, f) = \delta(k_x - (k^2 - (k_x^tx)^2)^{1/2} - (k^2 - (k_x^tx + k_x)^2)^{1/2})$$

$$C_i(k_x, z, f) = \int_{-\infty}^{\infty} \hat{p}_{tx(i)}(k_x^tx, f) \hat{p}_{rx(i)}(k_x^tx + k_x, f) H(k_x, z, k_x^tx, f) dk_x^tx$$
- K-space $I_i(k_x, k_z)$ of the image $I_i(x, z)$:

$$I_i(x, z) = \int_0^\infty p_{tx(i)}^*(x, z, f) p_{rx(i)}(x, z, f) df$$

$$= \int_0^\infty \int_{-\infty}^{\infty} C_i(k_x, z, f) e^{+j2\pi k_x x} dk_x df$$

$$I_i(x, z) = \int_0^\infty \int_{-\infty}^{\infty} \int_{-\infty}^{\infty} C_i(k_x, k_z, f) e^{+j2\pi k_x x} e^{+j2\pi k_z z} dk_x dk_z df$$

$$I_i(k_x, k_z) = \int_0^\infty C_i(k_x, k_z, f) df$$

FORWARD & INVERSE STOLT MAPPINGS

- Forward Stolt mapping from $k = \frac{f}{c}$ to k_z :**
 - $k_z = (k^2 - (k_x^tx)^2)^{1/2} + (k^2 - (k_x^tx + k_x)^2)^{1/2}$
- Inverse Stolt mapping from k_z to $k = \frac{f}{c}$:**
 - $k = \frac{1}{2k_z} (4k_x^tx(k_x^tx + k_x)(k_x^tx + k_z)^2 + (k_x^tx + k_z)^2)^{1/2}$
- Full k-space $I_i(k_x, k_z)$ of the image $I_i(x, z)$:

$$\hat{C}_i(k_x^tx, k_x, f) = \hat{p}_{tx(i)}^*(k_x^tx, f) \hat{p}_{rx(i)}(k_x^tx + k_x, f)$$

$$I_i(k_x, k_z) = \int_{-\infty}^{\infty} \hat{C}_i(k_x^tx, k_x, f) \left(\frac{c}{2k_z} (4k_x^tx(k_x^tx + k_x)(k_x^tx + k_z)^2 + (k_x^tx + k_z)^2)^{1/2} \right) dk_x^tx$$

WHY FOURIER BEAMFORMING?

- Pulse-echo ultrasound typically uses *delay-and-sum* (DAS) beamforming to coherently focus/image reflected signals
- Fourier beamforming* accelerates image reconstruction by taking advantage of well-known Stolt mappings in k-space (Figure 1)
 - Multistatic-FMC³, Plane-Wave⁴, Focused-Transmit FMC⁵

DEMONSTRATION IN FIELD II SIMULATIONS⁸

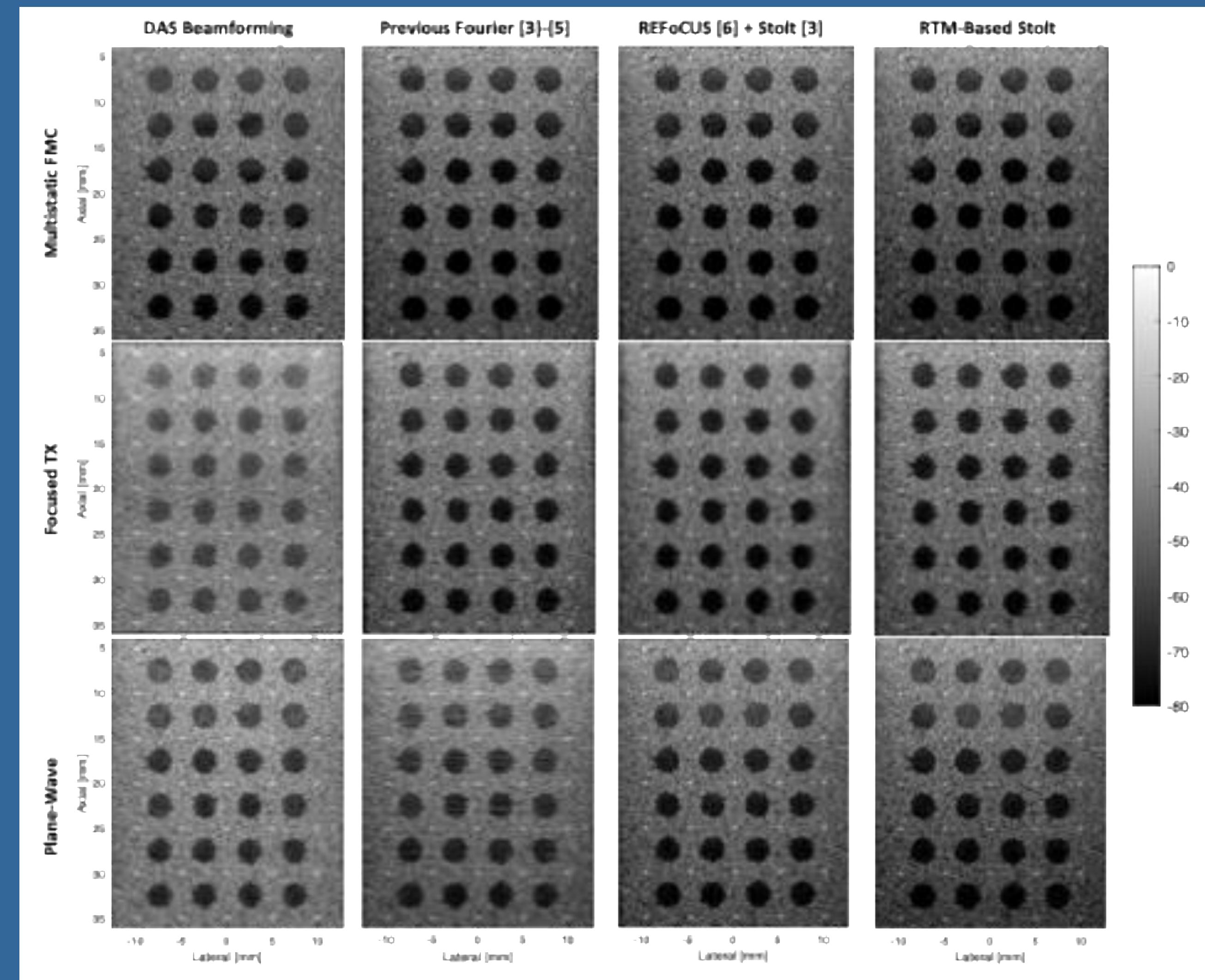


Figure 4. Visual comparison of RTM-based Stolt mapping to DAS beamforming, the previous Fourier beamformers³⁻⁵, and REFOCUS⁶ followed by the full multistatic Stolt mapping³ after recovering the full multistatic full-matrix capture (FMC) dataset.

CONCLUSIONS

- Both REFOCUS⁶+FMC Stolt³ and RTM-Stolt generalize well
- RTM-Stolt slower but reconstructs images from individual TX's
- Garcia² is less accurate than Lu⁴ (Figure 2) but more popular even though computation cost same—b/c Garcia² open-source
- <https://github.com/rehmanali1994/FastFourierBeamformers>

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