Developing a new test-bench for screening effective nextgeneration speech processing algorithms for cochlear implants.

Anaïs Donzeau¹; Tobias Goehring²; Yue Zhang¹; Manuel Segovia-Martinez¹

- ¹ Oticon Medical, Vallauris, France
- ² Cambridge Hearing Group, MRC Cognition and Brain Sciences Unit, University of Cambridge, UK

1. Introduction

Improving cochlear implant (CI) user's speech performance with new signal processing algorithms is a significant challenge faced by CI manufacturers. Clinical studies are used to test new proposals and determine whether they should be integrated into products. However, conducting such studies for every new proposal is not feasible due to time and cost constraints¹.

To address this issue, we propose another approach featuring an evaluation test-bench that helps to compare new CI signal processing designs by predicting speech performance improvements using intelligibility models.

Our evaluation test-bench aims to have a first set of metrics that may reflect the performance of CI users for speech in noise.

2. Materials

Total 114 audio files

- 19 tracks of clean speech
- 3 different languages
- Male and female speakers

| Speech in SNR | | | | Reverb & babble noise | Reverb & white noise |
|---------------|---|---|---|-----------------------|----------------------|
| 5dB SNR | X | X | | | X |
| 10dB SNR | X | | X | X | |

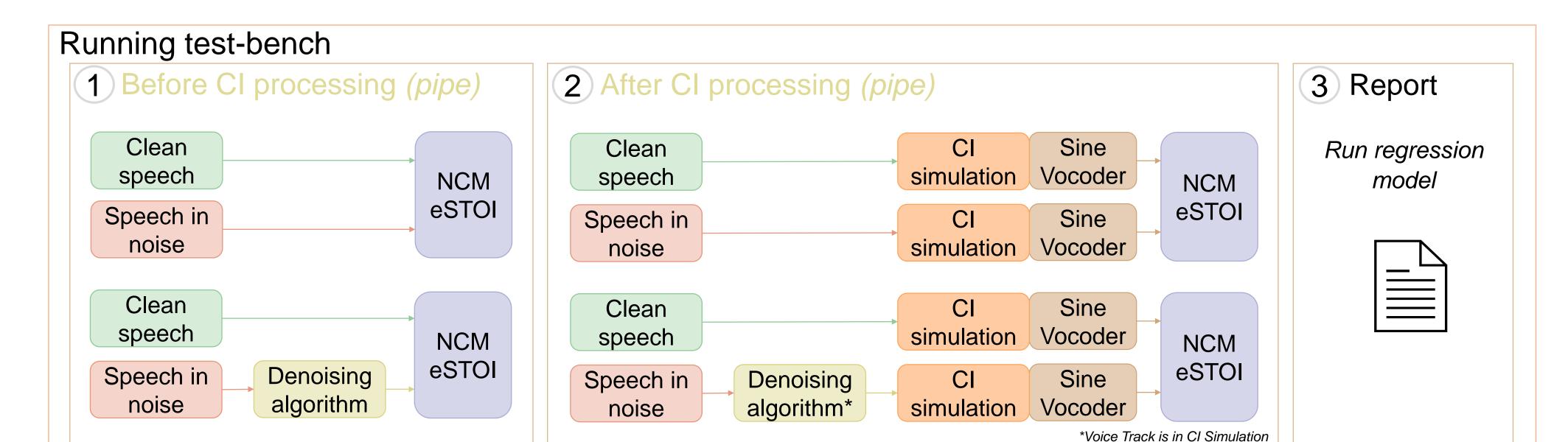
3. Method

Used Metrics

- eSTOI²: extended Short-Time Objective Intelligibility
- NCM³: Normalized Covariance Metric

Mixed effect logistic regression model

eSTOI = denoising algorithm + pipe + pipe * denoising algorithm + (1 noise: clean speech)NCM = denoising algorithm + pipe + pipe * denoising algorithm + (1 noise: clean speech)Random factors Fixed factors, with interaction Dependent variables



4. Results

Denoising algorithms

- Voice Track: Oticon Medical denoising solution for Neuro2 product⁴.
- SEDA iOS: denoising solution designed by York-Sound company⁵.
- Non causal DPRNN: non-causal Deep Neural Network (DPRNN)⁶⁻⁷
- Small DPRNN: non-causal DPRNN⁶⁻⁷ with small number of parameters and small training data set.
- Causal DPRNN: 5ms delay causal DPRNN⁶⁻⁷.
- ALG_B, ALG_C: Anonymized algorithms.

Regression model

eSTOI:

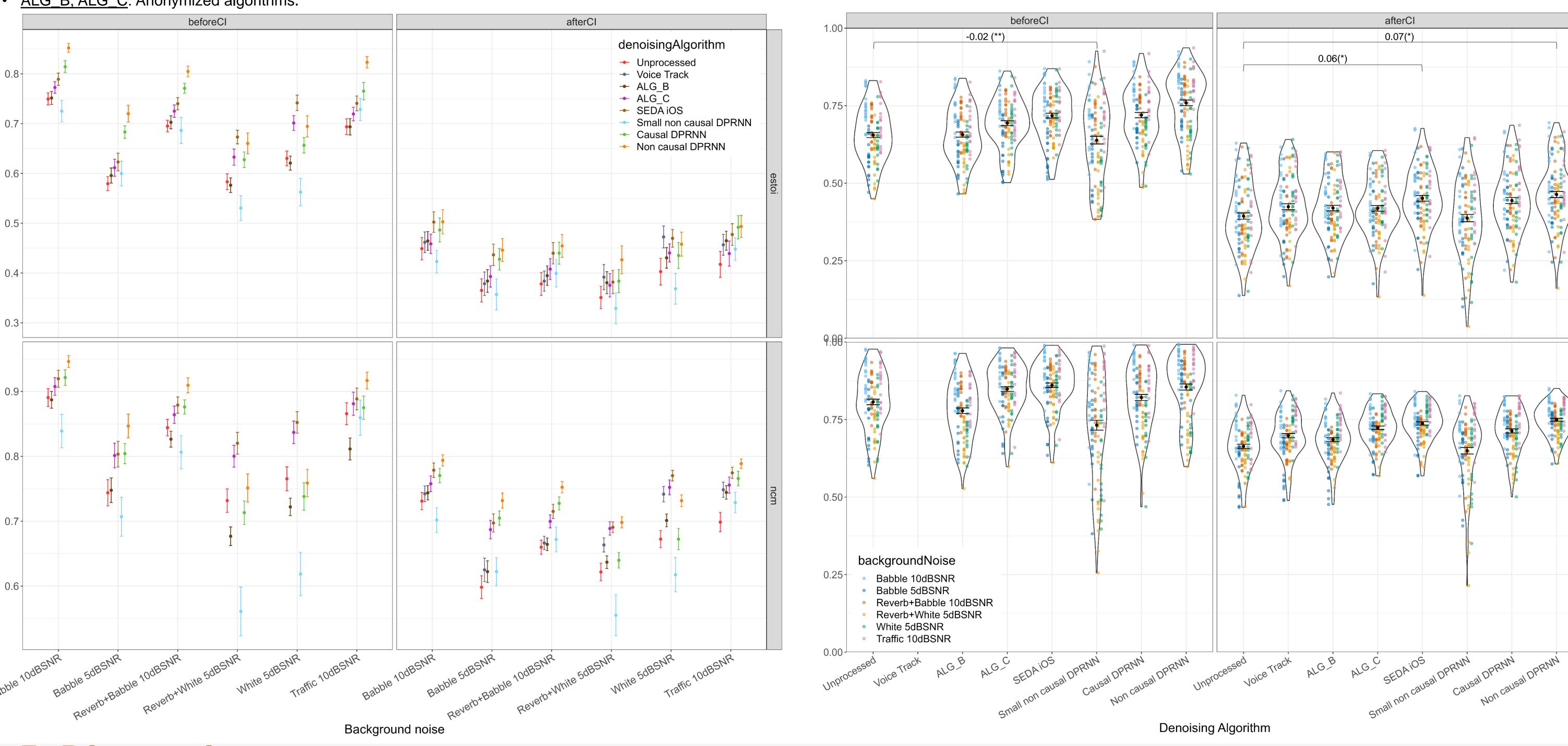
Denoising algorithm ($\chi^2=78.5$, df=7, p<0.001), pipeline ($\chi^2=1078.2$, df=1, p<0.001), denoising and pipeline ($\chi^2=40,0$, df=6, **p<0,001**).

- Small DPRNN is significantly worse than unprocessed before CI (β =-1.69, se=0.59, p<0.01).
- SEDA iOS is significantly better than unprocessed after CI (β =0.09, se=0.04, p<0.05).
- Non causal DPRNN is significantly better than unprocessed after CI (β =0.08, se=0.04, p<0.05).

NCM:

 $(\chi^2=98,2,$ Denoising algorithm df=7, p<0.001).

 Small DPRNN is significantly worse $(\beta = -2, 1,$ than unprocessed se=0.5, p<0.001).



5. Discussion

Preliminary conclusion

- Although eSTOI and NCM are not designed for CI, they are often used⁷⁻⁸ and we can see a **coherency of the results** between before and after CI:
 - Results indicate non causal DPRNN and SEDA iOS as the algorithms with significantly better intelligibility marker than Unprocessed
 - Results confirm Voice Track good performance with static noise
- In the current state, test bench can be used for algorithms comparison but not to predict patient performance
- eSTOI and NCM limitations:

Audiology 55.8 (2016): 431-438.

- Vocoders add variability (see poster M63: [1605])
- Markers not necessary linked to subjective preferences References

1 Carlyon, Robert P., and Tobias Goehring. "Cochlear implant research and development in the 21st century: A critical update." (2021)

3 As cited in: Chen, Fei, and Philipos C. Loizou. "Predicting the intelligibility of vocoded speech." Ear and hearing 32.3 (2011): 331

Improving the current test-bench

To increase the statistical power regression model:

- Need to generate more audio files
- Improve grouping of background noise to decrease the number of comparisons

hearing 41.6 (2020): 1492.

To improve robustness of the test-bench:

- More objective measures such as distortion
- Increase the variability of background noise
- Add MUSHRA subjective evaluation
- Run test-bench with different vocoders

Future work

- Better understand the result variability (eSTOI vs NCM, Before vs after CI)
- Confirm the approach by comparing test-bench results with listening tests on normal hearing using vocoders
- Validate the approach by comparing test-bench results with listening tests on Cl users
- Next generation Oticon Medical CI sound processor will implement the noise reduction selected with this test-bench

5 Soleymani, Roozbeh, Ivan W. Selesnick, and David M. Landsberger. "SEDA: A tunable Q-factor wavelet-based noise reduction algorithm for multi-talker babble." Speech communication 96 (2018): 102-115. 6 Luo, Yi, Zhuo Chen, and Takuya Yoshioka. "Dual-path rnn: efficient long sequence modeling for time-domain single-channel speech separation." ICASSP 2020-2020 IEEE International Conference on Acoustics, Speech and Signal Processing (ICASSP). IEEE, 2020. 7 Goehring, Tobias, et al. "Using recurrent neural networks to improve the perception of speech in non-stationary noise by people with cochlear implants." The Journal of the Acoustical Society of America 146.1

(2019): 705-718. 8 Lopez-Poveda, Enrique A., et al. "Speech-in-noise recognition with more realistic implementations of a binaural cochlear-implant sound coding strategy inspired by the medial olivocochlear reflex." Ear and

4 Guevara, Nicolas, et al. "The Voice Track multiband single-channel modified Wiener-filter noise reduction system for cochlear implants: patients' outcomes and subjective appraisal." International Journal of

2 Jensen, Jesper, and Cees H. Taal. "An algorithm for predicting the intelligibility of speech masked by modulated noise maskers." IEEE/ACM Transactions on Audio, Speech, and Language Processing 24.11

Oticon MEDICAL