



# Lab 3

## Pre-processing of ECG Signals: Notes

Meng-Lin Li (李夢麟), Ph. D.

[mlli@ee.nthu.edu.tw](mailto:mlli@ee.nthu.edu.tw)

Department of Electrical Engineering  
National Tsing Hua University

# 1. Order Selection of a FIR filter and Usage of fir1()

**fir1** FIR filter design using the window method.

**B = fir1(N,Wn)** designs an N'th order lowpass FIR digital filter and returns the filter coefficients in length N+1 vector B.

(impulse response)

The cut-off frequency Wn must be between  $0 < Wn < 1.0$ , with 1.0 corresponding to half the sample rate.

**B = fir1(N,Wn,'high')** designs an N'th order highpass filter.

You can also use **B = fir1(N,Wn,'low')** to design a lowpass filter.

Check frequency response via MATLAB **freqz()**  
MATLAB **filter()**?

$$\begin{aligned}
 y[n] &= -\sum_{k=1}^{\infty} a_k y[n-k] + \sum_{k=0}^M b_k x[n-k] \\
 &= y_{ss}[n] + y_{tr}[n] \\
 &= y_{zi}[n] + y_{zs}[n]
 \end{aligned}$$

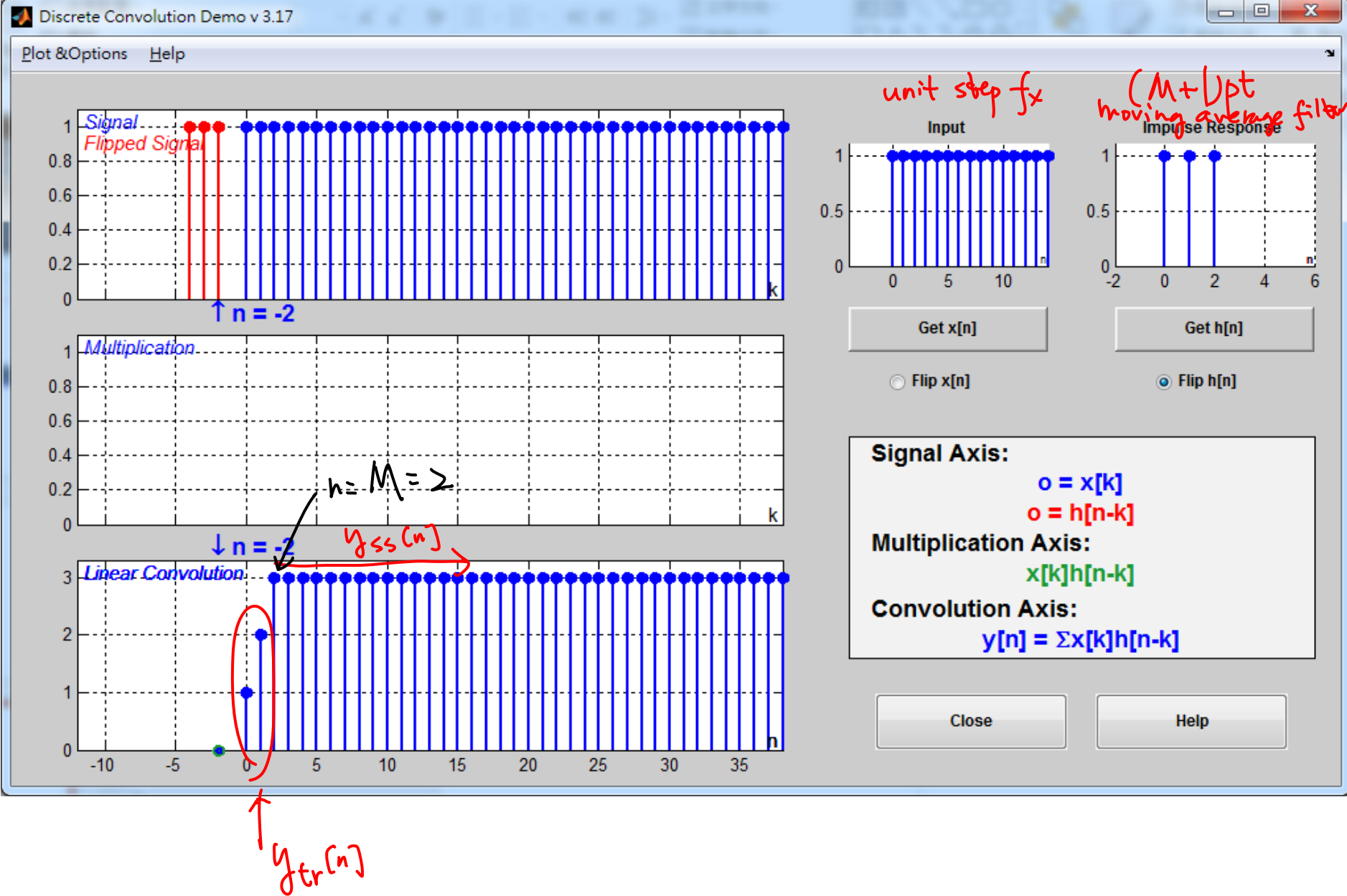
{	$y_{ss}[n]$ : <u>steady state</u> response	$y_{ss}[n] = \lim_{n \rightarrow \infty} y[n]$
	$y_{tr}[n]$ : <u>transient</u> response	$y_{tr}[n] = y[n] - y_{ss}[n]$

{	$y_{zi}[n]$ : zero input response	: the response due to initial conditions alone w/ the input set to 0. (i.e., $x[n]=0$ )
	$y_{zs}[n]$ : zero state response	: the response due to the system input w/ initial conditions set to 0 i.e., initially at rest, $y[n]=0, n < 0$

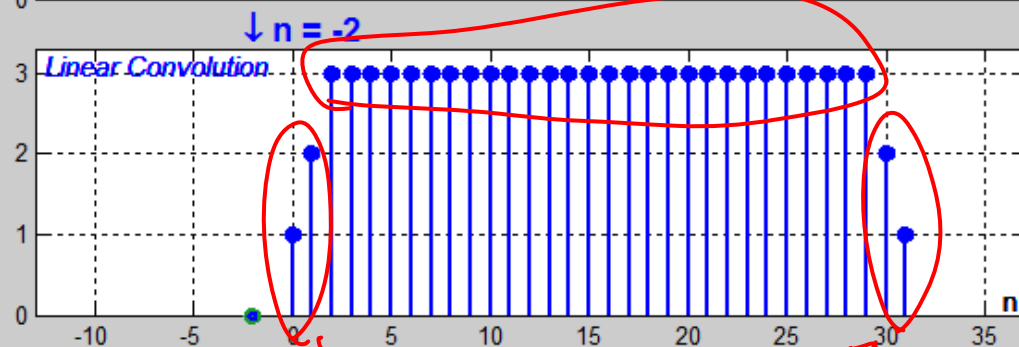
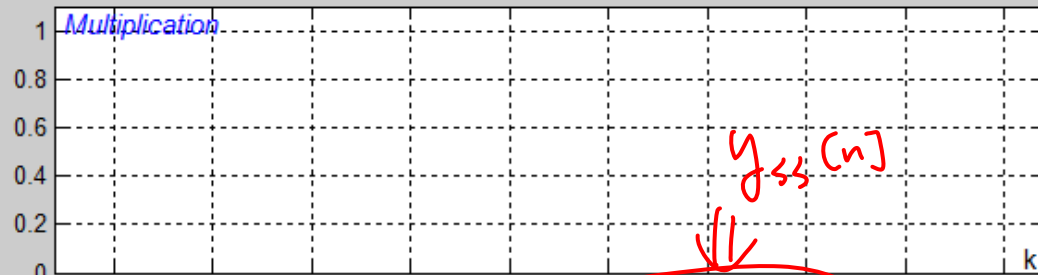
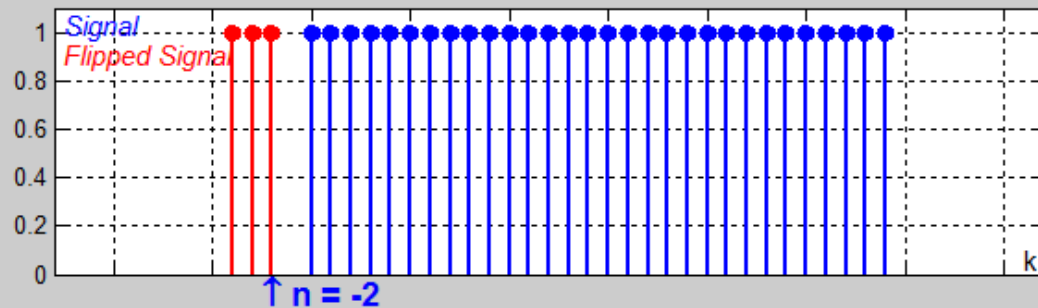
(see textbook p62-p64)

## More about LTI FIR Systems, Convolution Sum, Transient Response and Steady State Response

$$y_{ss}[n] = \lim_{n \rightarrow \infty} y[n]$$

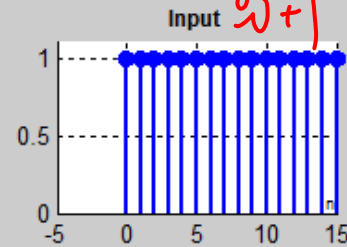
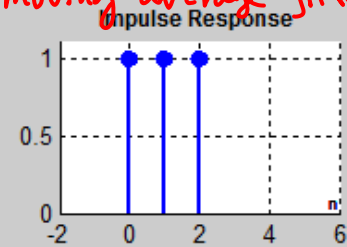


Plot &amp; Options Help



finite length  $N+1$

$(M+1)$  pt moving average filter

Get  $x[n]$ ☐ Flip  $x[n]$ Get  $h[n]$ ☒ Flip  $h[n]$ 

Signal Axis:

 $o = x[k]$  $o = h[n-k]$ 

Multiplication Axis:

 $x[k]h[n-k]$ 

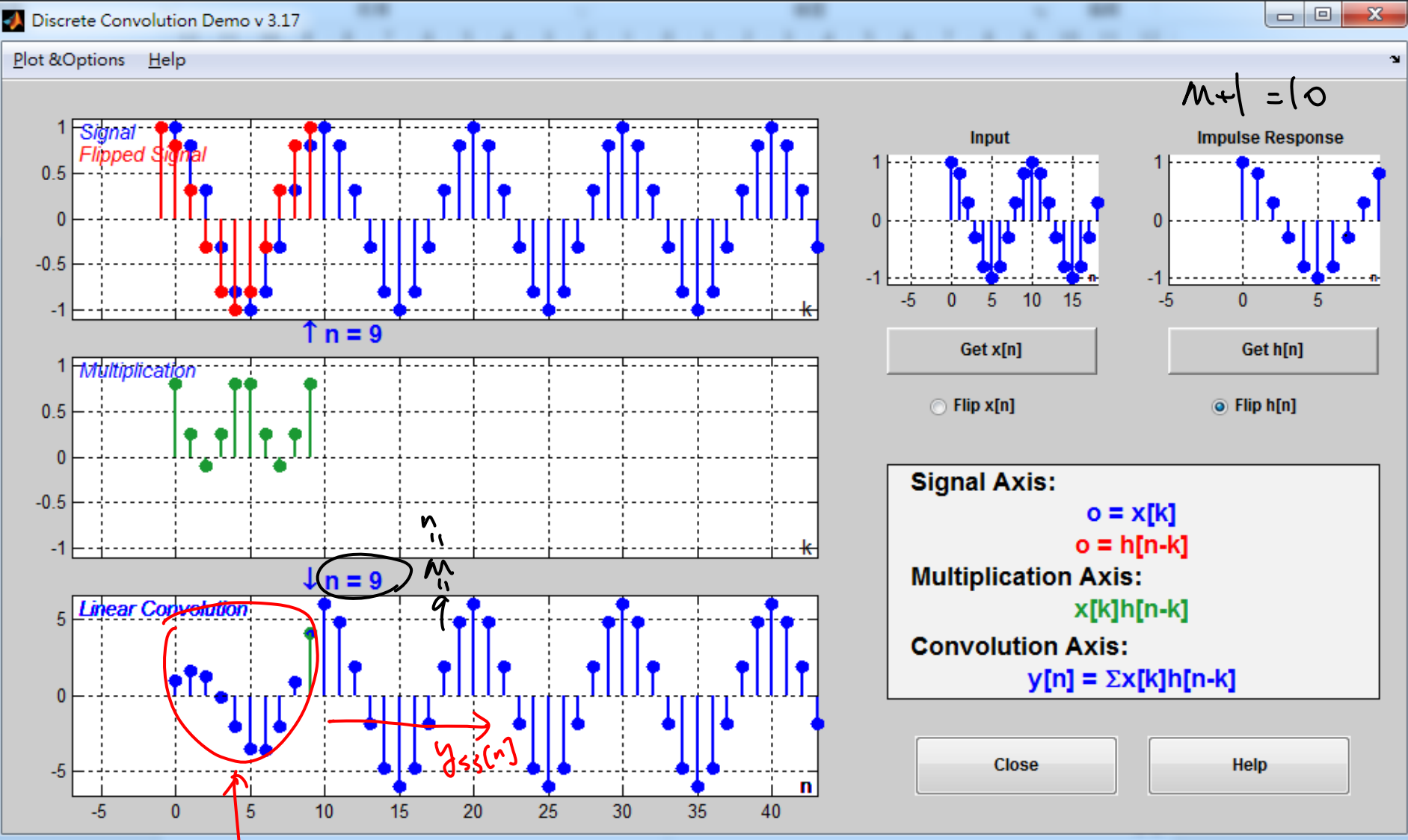
Convolution Axis:

 $y[n] = \sum x[k]h[n-k]$ 

Close

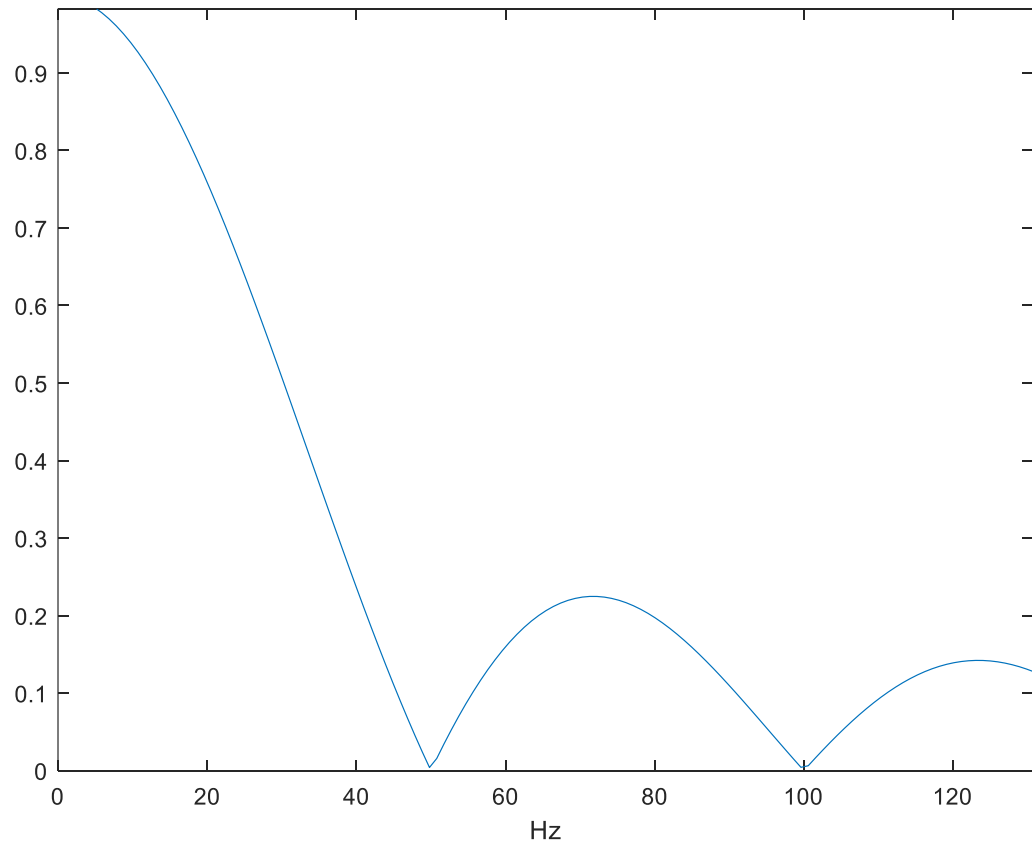
Help

what if  $(N+1) < (M+1)$ ?



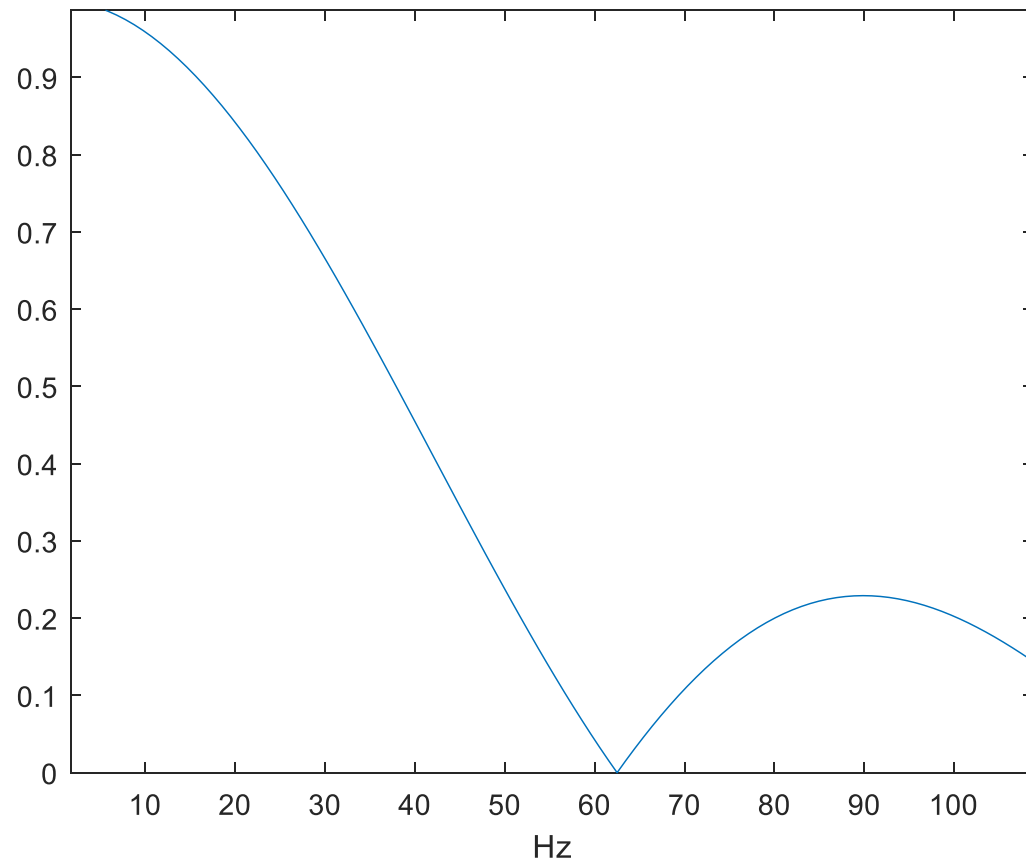
## 2. Moving Average Filtering and Difference Filtering

```
>> Fs = 500; % in Hz  
>> ma = ones(1,10)/10;  
>> figure  
>> plot((0:511)*Fs/512, abs(fft(ma,512)));  
>> xlabel('Hz')
```

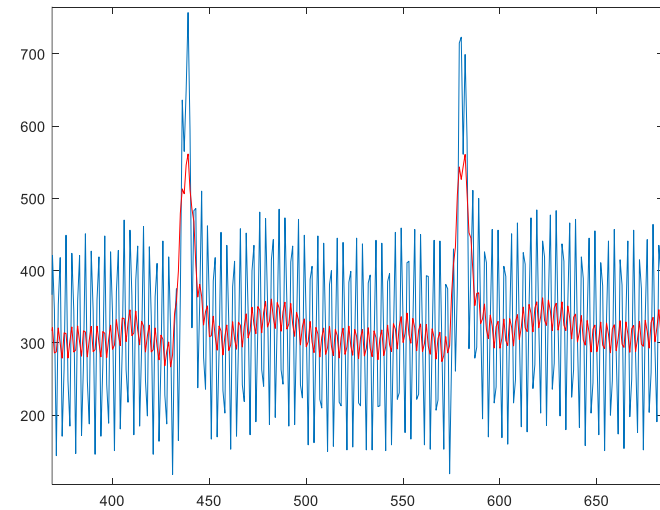




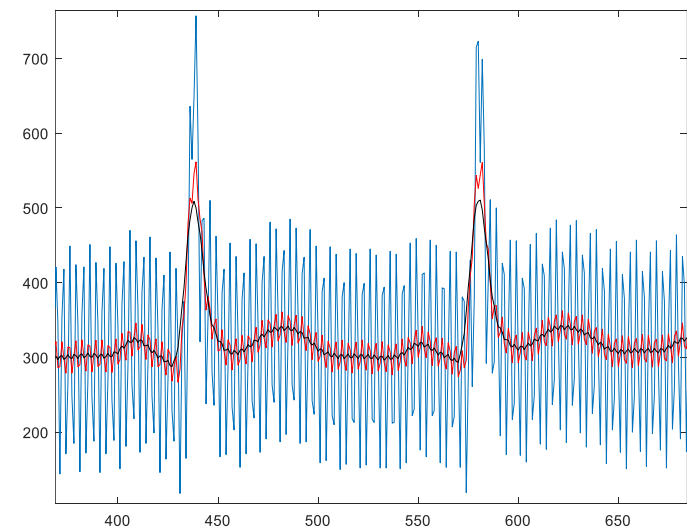
```
>> Fs = 500; % in Hz  
>> ma = ones(1,8)/8;  
>> figure  
>> plot((0:511)*Fs/512, abs(fft(ma,512)));  
>> xlabel('Hz')
```



```
ECG_notchfiltered = conv(raw_ECG,ma,'same');
```



```
ECG_notchfiltered = conv(ECG_notchfiltered ,ma,'same'); % cascaded system
```



# Fourier Transforms for DT Aperiodic Signals: View in Terms of DTFS

## Example 4.8

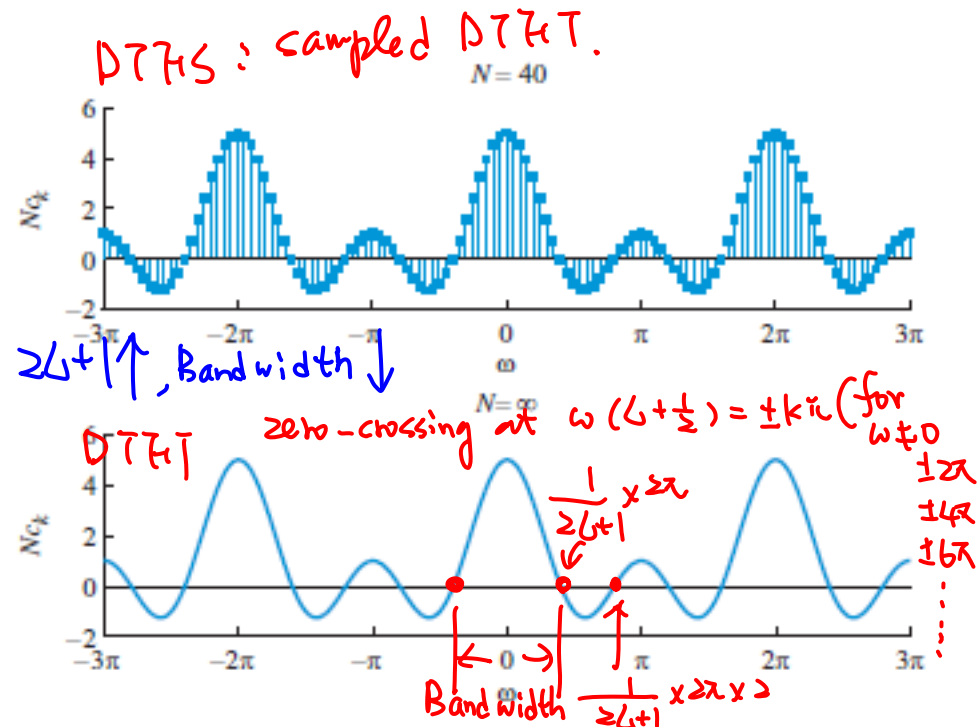
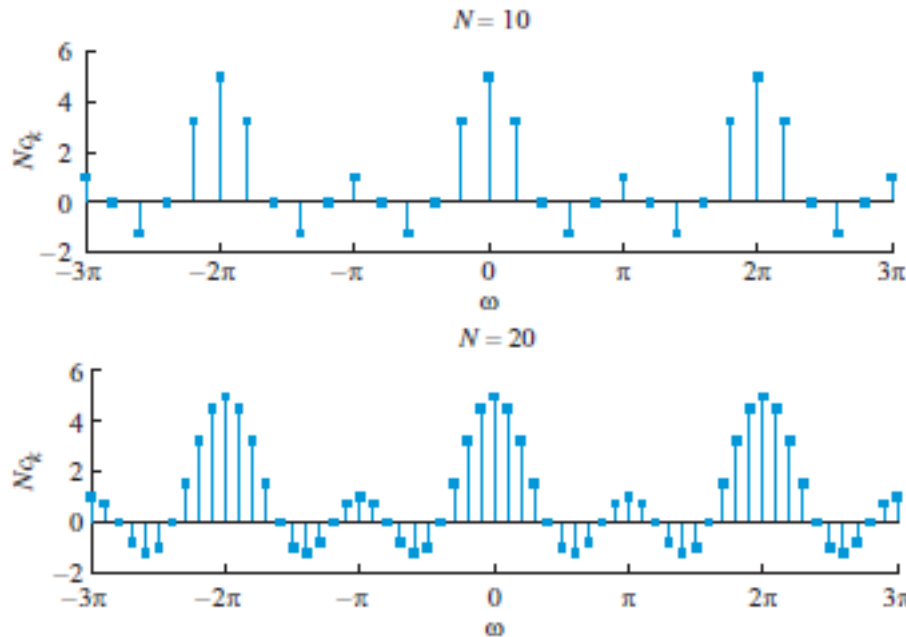


Figure 4.22 How the DTFS converges to the DTFT as the period  $N$  of a fixed-width ( $2L + 1 = 5$  samples) rectangular pulse tends to infinity.

$$\omega_k = (2\pi/N)k$$

from (4.19)  $\Rightarrow X(e^{j\omega}) = \begin{cases} 2L+1, & \omega = 0, \pm 2\pi, \pm 4\pi, \dots \\ \frac{\sin \omega(L + \frac{1}{2})}{\sin \omega/2}, & \text{otherwise} \end{cases}$

A plot of the discrete-time signal  $x[n]$  for  $L=2$ , showing a rectangular pulse of width 5 samples centered at  $n=0$ .