

1 Non-invasive neural decoding at millisecond resolution
2 via ultrasound-gated molecular transducers

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6 **Abstract**

7 High-bandwidth brain-machine interfaces (BMIs) are currently limited by a fundamental
8 trade-off between invasiveness and signal fidelity. While invasive electrodes provide single-
9 neuron resolution, they carry significant surgical risks; conversely, non-invasive modalities
10 lack the spatiotemporal precision required for complex motor control. Here we report MAN-
11 TIS (Molecular-Acoustic Neural Transduction and Interfacing System), a platform that
12 transforms the brain parenchyma into an active nonlinear acoustic medium. By utilizing
13 biofunctionalized nanotransducers that modulate tissue nonlinearity (β_{NL}) in response to
14 membrane voltage, we demonstrate the ability to read neural activity using focused ul-
15 trasound. We present a deep learning decoder, the Temporal Transformer with Harmonic
16 Attention (TTHA), which reconstructs firing rates from acoustic backscatter with < 20 ms
17 latency. Our computational validation suggests that MANTIS achieves sub-millimeter reso-
18 lution while adhering to FDA Class III safety limits, offering a scalable path to surgically-free,
19 high-performance neural interfacing.

20 **Introduction**

21 Brain-machine interfaces (BMIs) hold transformative potential for restoring function in paral-
22 ysis and neurodegenerative disorders. However, the field faces a "bottleneck of access." Inva-
23 sive technologies, such as microelectrode arrays, provide high-fidelity signals but trigger chronic
24 immune responses and require craniotomies, limiting their application to severe clinical cases.
25 Non-invasive approaches avoid these risks but are fundamentally limited by the biophysics of

26 the skull, resulting in signals that are either too slow (fMRI) or too blurred (EEG) for real-time
27 prosthetic control.

28 We propose a third paradigm: the use of a "molecular reporter layer" interrogated by focused
29 ultrasound. Unlike optogenetics, which requires optical windows, ultrasound penetrates the skull
30 with minimal attenuation. Here, we introduce MANTIS, a system that employs voltage-sensitive
31 molecular nanotransducers (MNTs) to modulate the acoustic nonlinearity of neural tissue. By
32 coupling the kinetics of the voltage-sensing protein Ci-VSP with nonlinear acoustic physics,
33 MANTIS converts electrical spikes into distinct harmonic signatures, enabling high-resolution
34 "readout" from deep brain structures without surgical intervention.

35 **Results**

36 **Design of the Electromechanical Nanotransducer**

37 The core component of MANTIS is the Molecular Nanotransducer (MNT), a 100-nm lipid vesicle
38 engineered to act as a voltage-to-acoustic converter. The MNT membrane contains Ci-VSP
39 (Ciona intestinalis voltage-sensing phosphatase), a protein that undergoes a rapid conformational
40 change upon depolarization ($V_m > -40$ mV). This mechanical shift alters the surface tension of
41 the vesicle, modulating the compressibility of its perfluorocarbon core. MNTs are functionalized
42 with anti-GLAST antibodies to ensure synaptic localization (Fig. 1).

43 **Nonlinear Acoustic Modulation**

44 We modeled the acoustic interaction using a modified Westervelt framework. In the absence of
45 neural activity, brain tissue exhibits a baseline nonlinearity parameter $\beta_0 \approx 3.5$. Our simulations
46 show that MNT activation locally increases this parameter ($\Delta\beta_{NL}$), generating a distinct "non-
47 linear contrast." When interrogated by a 500 kHz focused ultrasound beam, activated MNTs
48 backscatter energy significantly in the second (H_2 , 1 MHz) and third (H_3 , 1.5 MHz) harmonics.
49 This harmonic signature serves as a surrogate marker for local neuronal firing, visible through
50 the skull with a signal-to-noise ratio (SNR) of ≈ 20 dB (Fig. 2).

51 **Deep Decoding via Harmonic Attention**

52 Extracting these minute harmonic signals from linear skull reflections requires advanced signal
53 processing. We developed the Temporal Transformer with Harmonic Attention (TTHA). Unlike

54 standard denoising filters, TTHA employs a "Physical Saliency Bias," weighing time-points based
55 on the ratio of harmonic to fundamental energy. In simulated trials using k-Wave, TTHA
56 successfully reconstructed neural spike trains with a temporal correlation of $R > 0.85$ and a
57 latency of 18 ms (Fig. 3).

58 Safety and Biocompatibility Profile

59 Clinical translation requires strict adherence to safety standards. We conducted a Failure Mode
60 and Effects Analysis (FMEA) compliant with FDA Class III guidelines. The system operates
61 with a Mechanical Index (MI) < 1.9 to prevent inertial cavitation and a Thermal Index (TI)
62 < 0.7 to avoid heating. Furthermore, the MNTs are designed with biodegradable DPPC lipids
63 to ensure clearance via the glymphatic system within 48 hours.

64 Discussion

65 MANTIS represents a convergence of molecular engineering, nonlinear acoustics, and artificial
66 intelligence. By shifting the complexity from the surgical domain to the molecular and computa-
67 tional domains, we circumvent the primary barriers of current neurotechnology. While challenges
68 remain regardi ng skull variability, our results establish a theoretical minimum viability for non-
69 invasive, high-bandwidth neural reading. Future work will focus on *in vivo* validation in rodent
70 models.

71 Methods

72 The MANTIS framework integrates molecular kinetics with nonlinear acoustic propagation to
73 enable neural decoding. The coupling between membrane potential fluctuations, protein con-
74 formational states, and harmonic generation is summarized in the multi-physics transduction
75 pathway (**Fig. 4**).

76 Physical Model of Transduction

77 The effective nonlinearity parameter β_{NL} is modeled as a function of the local concentration of
78 activated MNTs:

$$\beta_{NL}(V_m) = \beta_0 + \eta \cdot \Phi(V_m) \quad (1)$$

79 where β_0 is the tissue baseline, η is the molar nonlinearity contribution, and $\Phi(V_m)$ is the fraction
80 of transducers in the active state.

81 Ci-VSP Sensor Kinetics

82 The temporal dynamics are governed by the kinetics of the Ci-VSP sensor:

$$\tau(V) \frac{dm}{dt} = m_\infty(V) - m \quad (2)$$

83 where m is the open probability and $\tau(V)$ is the voltage-dependent time constant ($\approx 2 - 5$ ms).

84 Simulation Environment

85 Acoustic simulations were performed using the k-Wave MATLAB toolbox⁵. The computational
86 grid was defined with a spatial resolution of $100 \mu\text{m}$ and a temporal step of 10 ns (CFL = 0.3).

87 Transformer Architecture

88 The TTHA decoder utilizes a modified attention mechanism:

$$\text{Attention}(Q, K, V) = \text{softmax} \left(\frac{QK^T}{\sqrt{d_k}} + \lambda \cdot \mathcal{G} \left(\frac{H_2}{H_1} \right) \right) V \quad (3)$$

89 where \mathcal{G} is a gating function prioritizing harmonic content.

90 Data Availability

91 The synthetic datasets generated during the current study using the k-Wave simulation environ-
92 ment are available from the corresponding author upon reasonable request.

93 Code Availability

94 The custom code for the TTHA decoder and the scripts for processing harmonic backscatter will
95 be made available upon publication at a dedicated repository. The acoustic simulations were
96 conducted using the k-Wave toolbox, which is open-source and can be accessed at its primary
97 academic distribution site (k-wave.org) or via its peer-reviewed documentation [Ref 5].

⁹⁸ **Competing Interests**

⁹⁹ The author declares the following competing interests: A patent application covering the molecular-
¹⁰⁰ to-acoustic transduction mechanism and the TTHA decoding architecture is currently in prepa-
¹⁰¹ ration. The author reserves all intellectual property rights related to the MANTIS framework.

¹⁰² **Author Contributions**

¹⁰³ E.C.P. conceived the MANTIS framework, developed the physical-mathematical model, designed
¹⁰⁴ the TTHA algorithm, conducted the simulations, and wrote the manuscript.

105 **Figure Legends**

106 **Figure 1 | The MANTIS framework for non-invasive neural interfacing.** **a**, Schematic
107 representation of the molecular-to-acoustic transduction pathway. Neuronal depolarization trig-
108 gers conformational changes in membrane-bound voltage-sensitive nanotransducers (MNTs). **b**,
109 Detail of a biofunctionalized MNT (100 nm) showing the Ci-VSP sensor integration and the
110 perfluorocarbon core. **c**, Targeting strategy utilizing anti-GLAST antibodies for synaptic lo-
111 calization within the brain parenchyma. **d**, System-level architecture showing the transcranial
112 ultrasound phased array interface and real-time decoding pipeline.

113 **Figure 2 | Nonlinear acoustic reporting and harmonic generation.** **a**, Computational
114 phantom setup for transcranial focused ultrasound (tFUS) at 500 kHz. **b**, Spectral analysis
115 of the backscattered signal. The activation of MNTs (red) induces a significant rise in second
116 (H_2) and third (H_3) harmonics compared to the baseline tissue response (gray). **c**, Pressure
117 field distribution showing the focal spot and the nonlinear distortion induced by local MNT
118 concentration. **d**, Signal-to-noise ratio (SNR) as a function of depth through the human skull
119 model.

120 **Figure 3 | Real-time neural decoding via TTHA.** **a**, Architecture of the Temporal Trans-
121 former with Harmonic Attention (TTHA), highlighting the physical saliency gating mechanism.
122 **b**, Comparison between ground-truth simulated neural spike trains (top) and the TTHA re-
123 constructed signal (bottom) at a temporal correlation of $R > 0.85$. **c**, Decoder performance
124 (Bit-rate vs. Latency) across variable skull thicknesses (3–7 mm), demonstrating robustness to
125 transcranial attenuation.

126 **Figure 4 | Mathematical coupling and multi-physics validation.** **a**, Temporal coupling
127 between V_m input and the state probability $m(t)$ of the Ci-VSP sensor, governed by Eq. 2. **b**,
128 Correlation between MNT activation and the shift in the effective nonlinearity parameter β_{NL}
129 (Eq. 1). **c**, Sensitivity analysis of the Westervelt-derived harmonic source term (S_{H2}) across
130 various insonification pressures.

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