

# Efficient deep learning model for mitosis detection using breast histopathology images

Monjoy Saha<sup>a</sup>, Chandan Chakraborty<sup>a,\*\*</sup>, Daniel Racocanu<sup>b,c,\*</sup>

<sup>a</sup> School of Medical Science and Technology, Indian Institute of Technology, Kharagpur, West Bengal, India

<sup>b</sup> Sorbonne University, Paris, France

<sup>c</sup> Pontifical Catholic University of Peru, Lima, Peru

## ARTICLE INFO

### Keywords:

Breast cancer  
Mitosis  
Deep neural network  
Handcrafted features  
Convolution  
Hematoxylin and eosin

## ABSTRACT

Mitosis detection is one of the critical factors of cancer prognosis, carrying significant diagnostic information required for breast cancer grading. It provides vital clues to estimate the aggressiveness and the proliferation rate of the tumour. The manual mitosis quantification from whole slide images is a very labor-intensive and challenging task. The aim of this study is to propose a supervised model to detect mitosis signature from breast histopathology WSI images. The model has been designed using deep learning architecture with handcrafted features. We used handcrafted features issued from previous medical challenges MITOS @ ICPR 2012, AMIDA-13 and projects (MICO ANR TecSan) expertise. The deep learning architecture mainly consists of five convolution layers, four max-pooling layers, four rectified linear units (ReLU), and two fully connected layers. ReLU has been used after each convolution layer as an activation function. Dropout layer has been included after first fully connected layer to avoid overfitting. Handcrafted features mainly consist of morphological, textural and intensity features. The proposed architecture has shown to have an improved 92% precision, 88% recall and 90% *F*-score. Prospectively, the proposed model will be very beneficial in routine exam, providing pathologists with efficient and – as we will prove – effective second opinion for breast cancer grading from whole slide images. Last but not the least, this model could lead junior and senior pathologists, as medical researchers, to a superior understanding and evaluation of breast cancer stage and genesis.

## 1. Introduction

Breast cancer (BC) is increasing gradually in developed and developing countries (considered second most common cancer among women) (Saha et al., 2016b, 2017). As per the Nottingham score, BC grading is done by the assessment of nuclear pleomorphism, tubule formation and mitotic count (Rakha et al., 2010). In the healthy breast, epithelial cell nuclei are uniform in size and shape. But in the case of malignancy, epithelial cell nuclei become non-uniform, darker and larger in shape. This transformation is called nuclear pleomorphism (Saha et al., 2016a). Tubule formation represents the percentage of malignant cells form regular duct structure. Mitotic count, one of the most important proliferation factors, carries significant diagnostic information required for BC histological grading. Indeed, it provides clues to estimate the aggressiveness and proliferation rate of the tumor (Elston and Ellis, 1991) by assessing the severity of the disease. During mitotic cell division, the chromosome is divided into two identical chromosomes. The mitotic cell division process is characterized by four

main phases: prophase, metaphase, anaphase and telophase (Mazia, 1961). Due to mutational changes in cell DNAs, there might be possibilities of uncontrolled cell division (King and Robins, 2006).

An individual observation area is usually called HPF (Irshad et al., 2013b). Mitotic scoring is calculated based on the number of mitotic figures present in the high power field (HPF). If 0–11 mitotic figures are present in 10 neighbour HPFs, then the score will be 1. If 12–22 mitotic figures are present in 10 neighbour HPFs, then the score will be 2, and the score will be 3 if more than 23 mitotic figures are visible in 10 neighbour HPFs (Elston and Ellis, 1991; Irshad et al., 2016).

In histopathological image analysis, automatic mitosis detection exhibits various challenges. Firstly, the shape of mitotic figures is different in each of the phases. Secondly, in hematoxylin and eosin (H&E) stained images, apart mitotic figures, some other similar objects like dense nuclei, lymphocytes, etc., are also present, inducing an important chance of misclassification. Therefore, due to some possible variation in the slide preparation (staining process, concentration, proportion, etc.), pathologists may miss some prominent mitotic figures. Moreover,

\* Corresponding author at: Pontifical Catholic University of Peru, Lima, Peru.

\*\* Joint corresponding author.

E-mail address: [daniraco@gmail.com](mailto:daniraco@gmail.com) (D. Racocanu).

manual detection of the mitotic figure is tedious and prone to intra-observer variability. Furthermore, in rural or urban areas with no/less expert pathologist, the manual assessment alone may provide wrong (or misleading) information. Automatic detection and count of the mitotic figure will not only attenuate these problems but also provide a safeguard to the doctors to consolidate their decision and support their commitment. In clinical practice, the pathologists assess the proliferated area present in the H&E stained tissue slides under  $40\times$  magnification.

Literature shows that computer aided mitosis detection (see MITOS-ATYPIA-14 (MITOS-ATYPIA, 2014) and MITOS 2012 (Roux et al., 2013; ICPR, 2012) challenges organized at ICPR) has not yet achieved enough performances (the maximum  $F$ -score gained was 0.734 in 2014) to envisage into routine implementation (Paul and Mukherjee, 2015). Therefore, an efficient and affordable deep learning model has been studied in this article. The proposed model is genuine and requires no prior knowledge about mitosis detection.

The key idea of the proposed architecture is based on two premises: (a) to learn deep learning features and handcrafted features from the ground truth annotated data and (b) classification between mitosis and non-mitosis. Small patches of size  $71 \times 71$  have been used to train the model. The use of small patches in the proposed model localizes the mitosis and non-mitosis in the images.

The paper is structured around VI sections: Section 1 gives an introduction. The literature review is reported in Section 2. Section 3 describes the dataset and proposed methodology. Results and discussion are discussed in Sections 4 and 5. Finally, Section 6 concludes and presents the perspectives of our work.

## 2. Literature review

Many automatic machine learning techniques are already developed in mitosis detection using H&E images and a certain success has been witnessed. Due to imperfections in cutting and staining, various issues arise from the variability of tissue appearance. Most of the mitosis detection techniques are based on conventional imaging techniques. From the extensive literature survey, we can remark that there are very few studies dedicated to the deep learning approaches. Table 1 shows the characterization of different mitosis detection methods using BC histological images. Table 2 illustrates comparative results of different BC dataset and strategies.

### 2.1. Review based on conventional techniques

Table 1 shows maximum BC mitosis detection issues which have been resolved by color, texture and intensity related attributes. Irshad

et al. (2013a) proposed a method where candidate cells were detected and segmented by extracting various channel features followed by Laplacian Gaussian, morphological operations and active contour (Irshad et al., 2013a). They used ICPR 2012 dataset. Their proposed method achieved  $F$ -score 72% on Aperio and 63% on Hamamatsu scanner images. This study was further extended based on various textures, Hierarchical Model and X (HMAX) features (Irshad et al., 2013b). This approach resulted in 0.76 recall, 0.75 precision and 0.76  $F$ -measure. The authors concluded that the result could be used for additional analysis. Irshad et al. (2014a,b) proposed spatial characterization and multispectral band selection technique for mitosis detection. Their algorithm achieved 67.35% detection rate and 63.74%  $F$ -score (Irshad et al., 2014a). The use of multispectral images using specifically designed spectral band selection algorithm for mitosis detection has been proposed in Irshad et al. (2014b). This algorithm achieved  $F$ -score 74%, positive predictive value 76% and true positive rate 74%.

In Huh et al. (2011), a probabilistic model using phase-contrast microscopy images has been discussed. The algorithm has been designed in a two-step processes: (a) the detection of spatiotemporal patches and (b) localization of birth events. The results show that their approach outperforms the previous approaches concerning computational efficiency and detection accuracy. In the method proposed by Tek et al. (2013), mitosis detection was done by extracting generic features and classifying by single and cascaded Adaboost classifier. The authors tested their model on ICPR 2012 contest dataset. The performance of the single classifier was 68% recall, 28.1% precision, 39.7%  $F$ -score, whereas, cascaded Adaboost classifier shows 54% recall, 62.7% precision, 58%  $F$ -score. The authors suggested to use the ensemble of cascaded Adaboost classifier rather than single classifier along with the features which express better color variations and granular structure.

Roux et al. (2013) described the methods used for MITOS @ ICPR 2012 contest dataset. The participants to this first challenge in Digital Pathology used level set, active contour, thresholding, mathematical morphology along with radiometry, morphological features and texture features for the detection of mitosis (Roux et al., 2013). The authors achieved  $F$ -measure 0.78 in mitosis detection. Liu et al. (2010) proposed the development of a mitosis event detection technique using hidden conditional random field. The model was designed into two parts. The candidate spatiotemporal sub-regions were segmented by image pre-conditioning and volumetric segmentation. This method achieved 85% recall and 95% precision (Liu et al., 2010). Schlachter et al. (2010) used harmonic filters with rotation invariant to detect mitosis in colorectal cancer images. Their approach successfully detected the mitosis in colorectal cancer (Schlachter et al., 2010).

Tao et al. (2007) proposed the use of a support vector machine classifier for mitotic figure detection using high-content screening data.

**Table 1**  
Categorization of mitosis detection approaches.

Categorize		Mitosis detection approaches
Hand-crafted features	Texture based	Co-occurrence features, scale-invariant features, run-length features (Liu et al., 2010) Wavelet-based (Dahl et al., 2013) Oriented gradient histograms [HOG] (Masci et al., 2011) Generic features (Huh et al., 2011) Blue ratio (Liu et al., 2010) Maximization of relative-entropy (Roux et al., 2013) Spectral band selection (Jia et al., 2014) Gamma-Gaussian Mixture Model (Sirinukunwattana et al., 2016) Chan-Vese level set (Deng et al., 2009) SCILAIM software used for mitosis detection using Feulgen Stained BC images (Saha et al., 2015) Learning based (Krizhevsky et al., 2012)
	Color-based	
Deep learning		Convolutional neural network (CNN) (Srivastava et al., 2014) Deep CNN and max-pooling (MITOS-ATYPIA, 2014) CNN and handcrafted features (Huh et al., 2011) CNN and seeded blob features (Malon et al., 2012) AggNet: deep learning from crowd (Albarqouni et al., 2016)

**Table 2**  
Comparative results of different dataset and methods.

Reference	Dataset used	F-score	Precision	Recall	Accuracy
Aptoula et al. (2013)	MITOS-ATYPIA-14	0.734	0.826	0.66	–
MITOS-ATYPIA (2014)	ICPR 2012 – Mitosis	0.782	0.88	0.70	–
Irshad et al. (2014a)	detection contest	0.70 (Aperio images), 0.56 (Hamamatsu images)	0.74 (Aperio images), 0.71 (Hamamatsu images)	–	–
Malon et al. (2012)		0.659	0.74	0.59	–
Sirinukunwattana et al. (2016)		0.513	0.46	0.57	–
Huh et al. (2011)		0.397	0.28	0.68	–
Krizhevsky et al. (2012)		0.374	0.14	0.80	–
Irshad et al. (2013a)		0.7345	0.84	0.65	–
Liu et al. (2010)		0.76	0.75	0.76	–
Schlachter et al. (2010)		0.34	–	–	–
Tao et al. (2007)		0.64	–	0.67	–
Nateghi et al. (2014)		–	–	–	0.84
Üstüner and Bilgin (2015) and Tripathi et al. (2013)		0.7094 (Aperio images), 0.7011 (Hamamatsu images)	–	–	–
Irshad et al. (2014b)		0.7847	0.80	0.77	–
Roullier et al. (2011)		0.74	0.76	–	–
Cireşan et al. (2013)		–	–	–	0.859
Roullier et al. (2011)		–	0.7304	0.8235	–
Dahl et al. (2013)		–	–	0.8680	0.8794
Irshad et al. (2013a)	AMIDA13	0.319	–	–	–
Chang et al. (2012)		0.6133	–	–	0.8695

The model tested on 99 cells and result shows 95.2% sensitivity and 95.8% specificity (Tao et al., 2007). Another computerized mitosis detection technique has been described in Malon et al. (2012). The authors found strong agreement between pathological observation results and computerized technique. In Huang and Lee (2012), Exclusive Independent Component Analysis has been used for mitosis detection. The algorithm tested on ICPR 2012 dataset. They achieved an area under the curve 100%. In Tashk et al. (2013), objective and texture based features have been used for mitosis detection. The acquired histology images firstly pre-processed by 2D anisotropic diffusion and morphological operations. Secondly, maximum likelihood estimation had been used for pixel-wise feature extraction. Finally, a SVM classifier has been used for classification. The test has been done on ICPR 2012 contest dataset images and achieved *F*-score of 70.11% for Hamamatsu images and 70.94% for Aperio XT scanner images. The work has been extended in Tashk et al. (2014). Nateghi et al. (2014) present an automatic mitosis detection method using cast function and Genetic optimization algorithm. The segmented mitosis and non-mitosis cells were classified using the SVM classifier. They achieved *F*-score 78.47% (Nateghi et al., 2014). In Üstüner and Bilgin (2015), statistical detection algorithms, i.e., constrained energy minimization, matched filtering and adaptive coherence estimator has been used for mitosis detection. They used matched filter and achieved 80% accuracy.

In Giusti et al. (2014), the authors compared the manual and automatic mitosis detection algorithms. They suggested that there should be a sufficient number of the training dataset. Tripathi et al. (2013) proposed a 2-Sieve model for mitosis detection. They have extracted Gray Level Entropy Matrix features and Multiresolution wavelet features on all the spectral bands. Classical data mining technique and dimensionality selection technique had been used in this model. Their results show positive predictive value 73.04% and sensitivity 82.35% (Tripathi et al., 2013). The approach presented in Roullier et al. (2011), uses the whole slide histological images for mitotic cell extraction and visualization, using the multi-resolution graph-based technique. The accuracy of this unsupervised learning technique was improved by spatial refinement of label regularization.

In Sharma et al. (2015), the authors reviewed the graph-based methods for microscopic histopathology images. They addressed various methodologies and their corresponding time complexities. The authors concluded that graph based methods are capable of differentiating tissue component based on neighborhood relationships and spatial

arrangements. This tends to consume less time during training and testing phase. The authors of Kayser et al. (2016) proposed structure and function based diagnosis using tissue slides. They used histological images for measuring staining intensity in a gray level. Additionally, Shannon's and structural entropy and entropy flow had been derived from the mapped gray level datasets. The significant changes found in the entropy level suggested biological function and structure based diagnosis for rapid reporting and result.

## 2.2. Review based on convolution and deep learning techniques

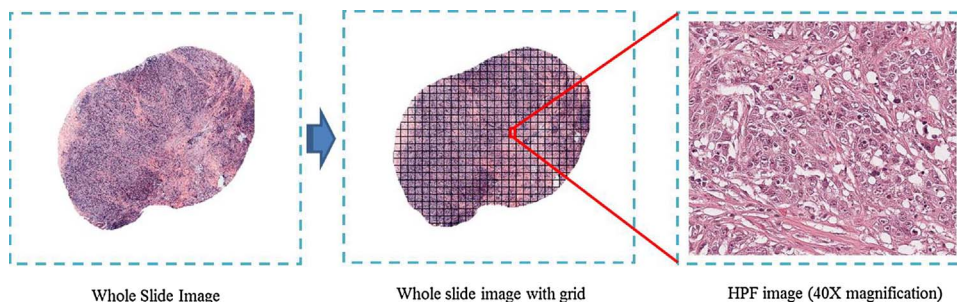
A deep neural network based mitotic figure detection technique was proposed for BC histology images (Cireşan et al., 2013). This study was based on the deep max-pooling convolutional network. Their approach won the ICPR 2012 mitosis detection challenge by achieving an *F*-score of 0.782. Veta et al. (2016) reported an assessment of object-level inter-observer variability on mitosis counting in BC (Veta et al., 2016). The authors trained a deep learning model for mitosis counting followed by performance analysis based on an inter-observer agreement between automatic and manual method. Their framework consisted of four convolutional and two fully connected layers. The authors employed AMIDA13 dataset with image patch of size  $63 \times 63$ . They concluded that small objects create substantial disagreement so there should be size constraint in mitosis detection. The results of AMIDA13 challenge algorithms of 11 participants have been summarized in Veta et al. (2015) and the outcomes of individual participants are discussed.

Wang et al. (2014a,b) used CNN and handcrafted features for mitotic figure detection. The proposed model employs one convolution, one pooling and one fully-connected layer. The convolution layer contains 64 neurons; the pooling layer comprises of 128 neurons and the fully-connected layer contains 256 neurons. The parameters of the each layer were fixed, i.e.  $8 \times 8$  convolution kernel size,  $2 \times 2$  pooling kernel size. The handcrafted features used in the model are morphological (eccentricity, area, compactness, smoothness, etc.), textural (concurrence features and run-length features) and intensity features (median, mean, variance, interquartile range, maximum/minimum ratio, range, etc.). They tested the model on ICPR 2012 dataset and achieved *F*-measure of 0.7345. Another CNN based mitosis detection technique has been described in Malon et al. (2013). They used CNN based feature along with nuclear features in this model. They tested on the ICPR 2012 dataset and achieved *F*-score 0.589 on the multispectral

**Table 3**

The 55 Hand-crafted features extracted from the mitosis and non-mitosis image patches.

Sl. No.	Features	Mitosis	Non-mitosis
1	Area*	7.475 ± 1.769	9.022 ± 2.246
2	Perimeter*	27.595 ± 6.936	31.824 ± 6.304
3	Compactness	112.158 ± 22.610	113.890 ± 23.592
4	Eccentricity	0.841 ± 0.189	0.824 ± 0.210
5	Zernike moment	NaN	NaN
6	Area equivalent diameter	8.973 ± 0.949	8.974 ± 1.134
7	Perimeter equivalent diameter*	16.919 ± 4.005	20.4224 ± 5.084
8	Form factor*	0.334 ± 0.042	0.115 ± 0.024
9	Convex area*	66.694 ± 16.807	79.319 ± 17.696
10	Solidity*	0.852 ± 0.050	0.405 ± 0.059
11	Roundness*	0.658 ± 0.123	0.375 ± 0.114
12	Aspect Ratio*	1.395 ± 0.254	1.057 ± 0.273
13	Concavity*	11.540 ± 5.669	15.160 ± 4.733
14	Rectangularity	0.698 ± 0.040	0.682 ± 0.059
15	Fourier descriptor*	62,007.048 ± 16,264.126	70,987.962 ± 12,160.941
16	Mean intensity	1.844 ± 0.293	1.798 ± 0.358
17	Energy	1.825 ± 0.291	1.842 ± 0.354
18	Homogeneity	2.237 ± 0.292	2.267 ± 0.354
19	Spot area ratio	2.827 ± 0.289	2.787 ± 0.384
20	Contour, irregularity	0.165 ± 0.223	0.242 ± 0.356
21	Area irregularity	0.223 ± 0.068	0.218 ± 0.067
22	Area overlapped, ratio	0.177 ± 0.056	0.179 ± 0.089
23	Euler number	0.218 ± 0.067	0.223 ± 0.066
24	Extent	0.775 ± 0.041	0.281 ± 0.081
25	Major axis length	0.796 ± 0.052	0.800 ± 0.044
26	Minor axis length	0.757 ± 0.043	0.754 ± 0.061
27	Average radial ratio	0.704 ± 0.048	0.705 ± 0.051
28	Hausdorff dimension*	15.168 ± 0.389	10.743 ± 0.056
29	Smoothness*	13.326 ± 7.901	26.354 ± 9.227
30	Standard distance, ratio*	14.540 ± 8.038	23.871 ± 8.004
31	Autocorrelation*	13.460 ± 7.623	26.104 ± 8.834
32	Contrast*	33.699 ± 1.460	24.098 ± 8.166
33	Correlation-1*	3.370 ± 1.342	6.602 ± 1.249
34	Correlation-2*	3.605 ± 1.361	6.203 ± 1.174
35	Cluster Prominence	3.395 ± 1.290	3.576 ± 1.229
36	Cluster Shade	0.095 ± 0.028	0.105 ± 0.034
37	Dissimilarity	0.125 ± 0.035	0.114 ± 0.044
38	Skewness *	0.502 ± 0.029	0.927 ± 0.033
39	Entropy*	0.322 ± 0.034	0.814 ± 0.039
40	Homogeneity	0.600 ± 0.077	0.605 ± 0.095
41	Maximum probability	0.675 ± 0.079	0.662 ± 0.097
42	Sum of squares	0.617 ± 0.077	0.603 ± 0.092
43	Sum average	0.676 ± 0.078	0.692 ± 0.096
44	Sum variance*	0.798 ± 0.178	1.008 ± 0.209
45	Sum entropy	0.948 ± 0.178	0.957 ± 0.219
46	Difference variance	0.978 ± 0.168	0.963 ± 0.200
47	Difference entropy	0.054 ± 0.176	0.057 ± 0.212
48	Information measure of correlation-1	0.962 ± 0.010	0.958 ± 0.012
49	Information measure of correlation-2	0.952 ± 0.013	0.949 ± 0.016
50	Inverse difference homogeneity	0.960 ± 0.011	0.955 ± 0.012
51	Inverse difference normalized	0.943 ± 0.013	0.941 ± 0.014
52	Inverse difference moment normalized*	0.824 ± 0.052	0.467 ± 0.067
53	Maximum ratio*	0.815 ± 0.053	0.359 ± 0.069
54	Minimum ratio*	0.822 ± 0.051	0.566 ± 0.065
55	Haralick feature*	0.816 ± 0.053	0.459 ± 0.068

**Fig. 1.** High power field image (40× magnification) generation.



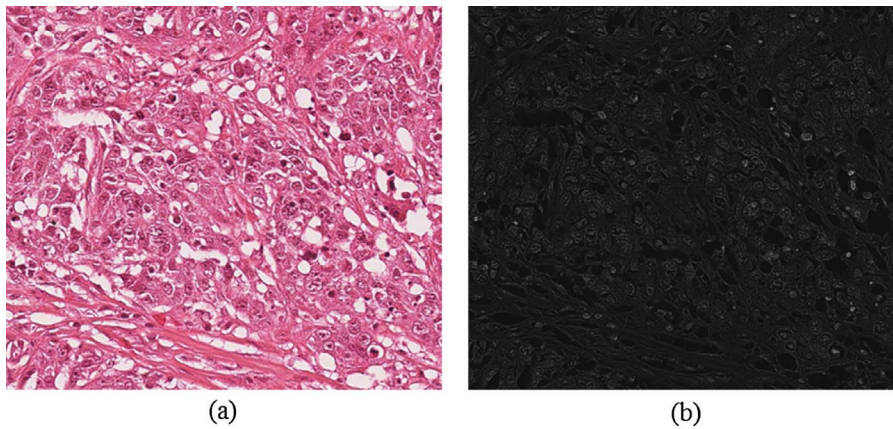


Fig. 2. RGB to blue ratio image conversion (a) original RGB image; (b) blue ratio image.

Table 4  
Proposed deep learning architecture.

Layer	Type	Maps	Neurons	Filter size
0	Input image	3	$71 \times 71$	–
1	Conv	90	$70 \times 70$	$2 \times 2$
2	Max-pooling	90	$35 \times 35$	$2 \times 2$
3	Conv	256	$32 \times 32$	$4 \times 4$
4	Max-pooling	256	$16 \times 16$	$2 \times 2$
5	Conv	384	$14 \times 14$	$3 \times 3$
6	Max-pooling	384	$7 \times 7$	$2 \times 2$
7	Conv	512	$6 \times 6$	$2 \times 2$
8	Max-pooling	512	$3 \times 3$	$2 \times 2$
9	Conv	512	$2 \times 2$	$2 \times 2$
10	FC-1	–	1000	$1 \times 1$
11	FC-2	–	2	$1 \times 1$

scanner and  $F$ -score 0.659 on the color scanner. They concluded that this technique provides majority mitosis with fair precision value (0.747 in Aperio, 0.759 in Hamamatsu and 0.738 in the multispectral scanner). In Albarqouni et al. (2016), convolutional neural network along with additional aggregation layer for learning from crowds have been employed for mitosis detection. The methodology used AMIDA13

Challenge BC histopathology image dataset achieved an overall  $F1$ -score of 0.433, a precision of 0.441 and a recall of 0.424.

Unlike most of the deep learning models involving convolutional, resizing and handcrafted layers, the approach presented in this paper employs deep learning for high-level feature learning. In our proposed deep architecture, the size of mitosis as well as non-mitosis patches were assigned the pixel size of  $71 \times 71$  at  $40\times$  magnification. Every patch contains only a single object, i.e. mitosis or non-mitosis, that would be suitable for the building of a supervised deep learning model. Therefore, we included handcrafted features instead of only deep learning network (DLN). On the other hand, to extract some additional features, handcrafted features are trained in a supervised fashion. Moreover, this supervised technique is much more efficient than the usual deep learning techniques. This method permits us to detect mitosis and non-mitosis efficiently from the large cohort of BC histological images.

The novelties of this paper are:

- The proposed deep architecture is efficient to learn and classify from a large number of non-annotated histological image data.
- The handcrafted features have been merged with the DLN features

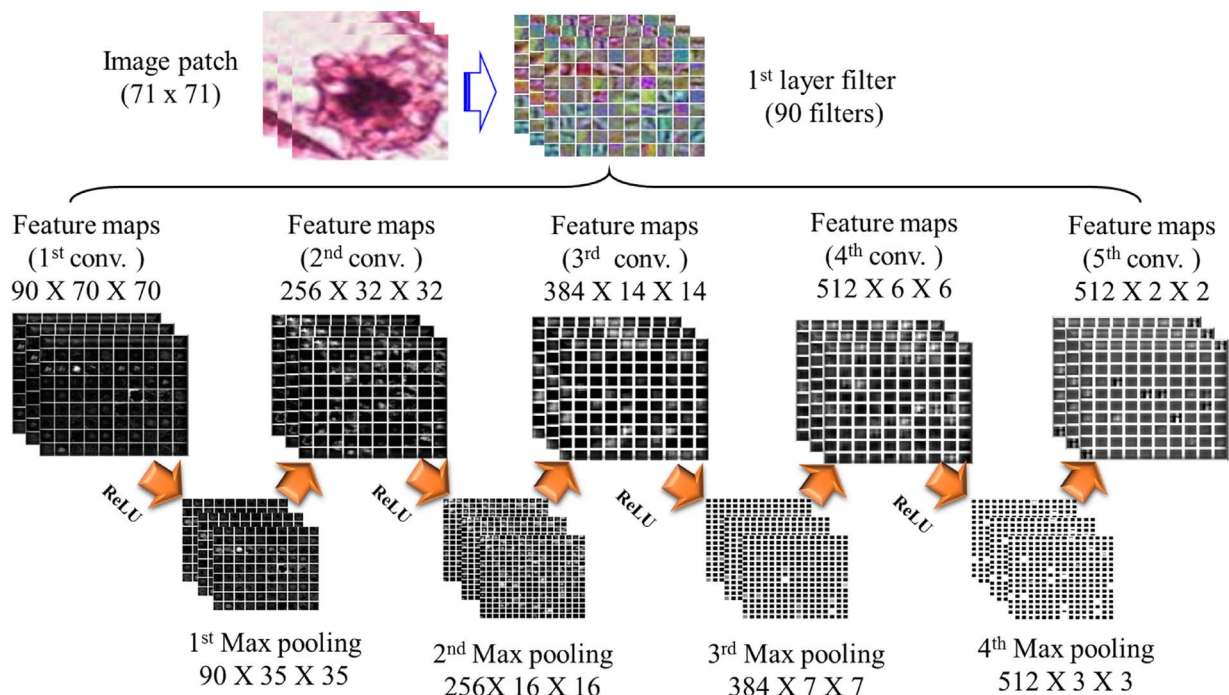


Fig. 3. Flow diagram of the proposed deep learning network.

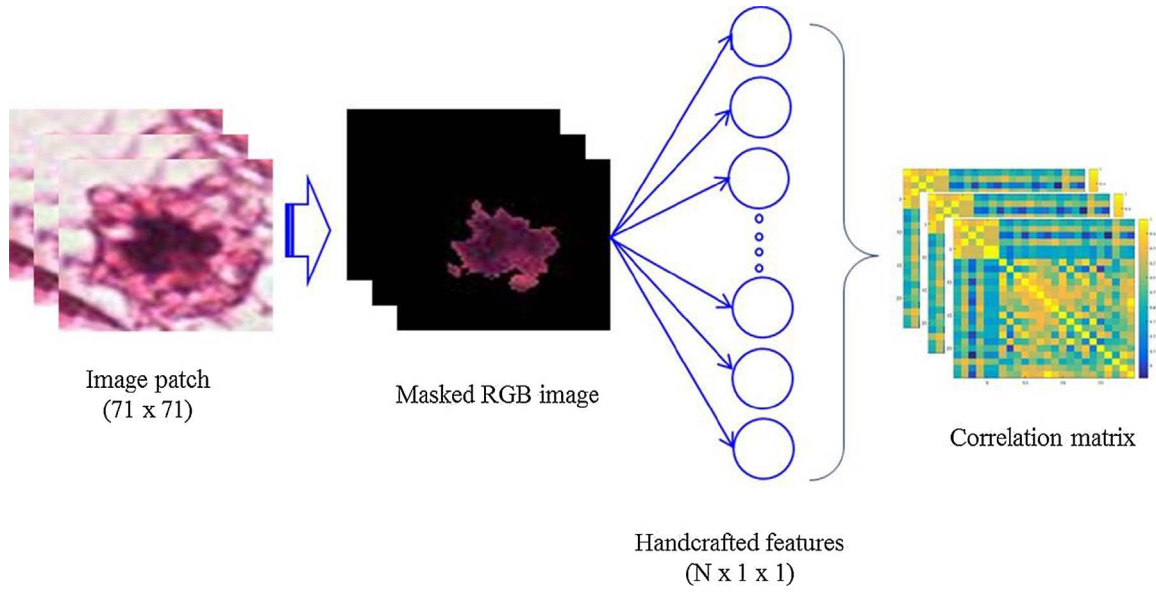


Fig. 4. Work flow diagram of the handcrafted features generation.

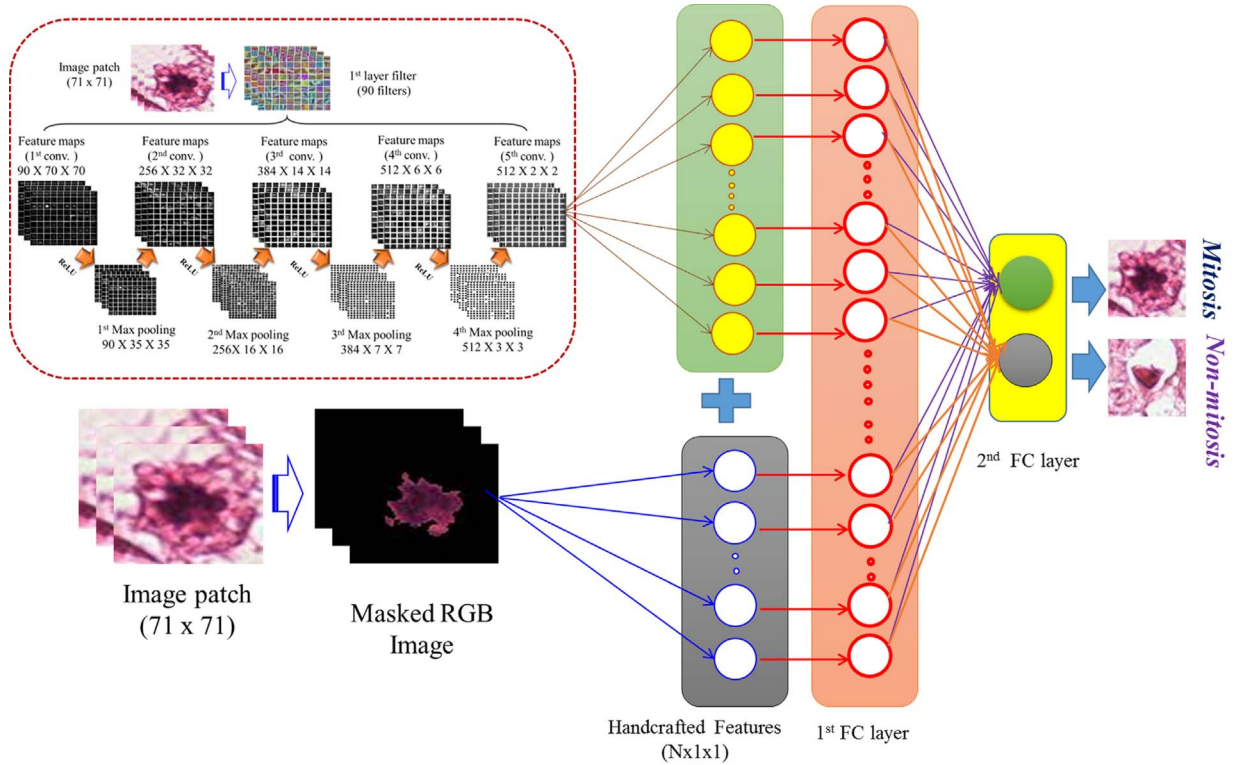


Fig. 5. Flow diagram of the proposed methodology.

and all the features directly fed to the first fully connected layer which represents high-level representation of mitosis and non-mitosis.

- Handcrafted layer allows quick traversal through large images for detection of single mitosis more accurately and efficiently.

To summarize, this paper incorporates the handcrafted features and deep learning based high-level features for mitosis detection. Our proposed approach is efficiently detecting mitosis patches from whole slide HPF images.

### 3. Experimental setup

#### 3.1. Dataset

The proposed method has been assessed on the MITOS-ATYPIA-14 (1,136 training and 991 testing frames), ICPR-2012 (35 training and 15 testing frames) and AMIDA-13 (326 training and 259 testing frames) dataset (MITOS-ATYPIA, 2014; ICPR, 2012; AMIDA, 2013). The slides were stained with routine H&E stain. The images were scanned by Hamamatsu NanoZoomer 2.0-HT and Aperio Scanscope XT. The size of MITOS-ATYPIA-14 images were for Aperio scanner  $1539 \times 1376$  pixels (*width*  $\times$  *height*), 1 pixel =  $0.2456 \mu\text{m}$  and Hamamatsu scanner

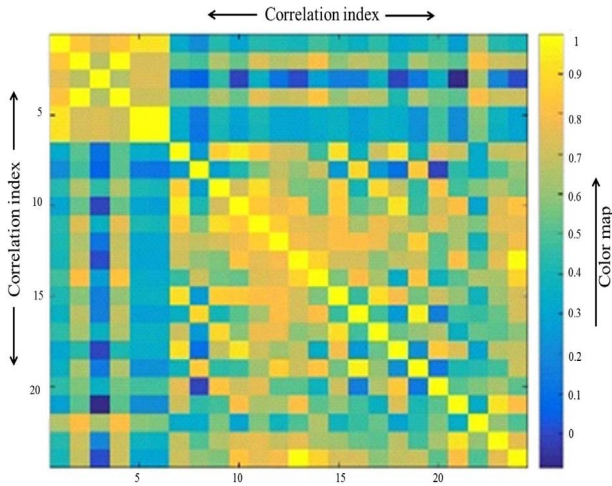


Fig. 6. Correlation matrix for 24 global features for image classification.

1663 × 1485 pixels (*width* × *height*), 1 pixel = 0.2273 μm. The size of ICPR-2012 images were for Aperio 2048 × 2048 pixels (*width* × *height*), 1 pixel = 0.2456 μm and Hamamatsu scanner 2252 × 2250 pixels (*width* × *height*), 1 pixel = 0.2273 μm. The size of AMIDA-13 images were for Aperio scanner 2000 × 2000 pixels (*width* × *height*), 1 pixel = 0.2456 μm. For all the dataset images, dimension is different, but magnification (40×) and pixel resolution are fixed, for a particular type of scanner.

### 3.2. Deep learning

#### 3.2.1. Convolutional network (CN)

It is an arrangement of an order of hidden layers. Let's, CN denoted by '*f*' and order of '*l*' layers/functions (*f*<sub>1</sub>, *f*<sub>2</sub>, *f*<sub>3</sub>, ..., *f*<sub>l</sub>) that feed to the input '*w*' vector to an output '*x*' vector. Mathematically, we can write (Sirinukunwattana et al., 2016; Lo et al., 1995; O'Brien et al., 2007):

$$x = f(w; v_1, v_2, v_3, \dots, v_l) \\ = f_1(., w_1) \circ f_2(., w_2) \circ \dots \circ f_{l-1}(., w_{l-1}) \circ f_l(., w_l) \quad (1)$$

Here, '*v<sub>l</sub>*' represents weight and bias vector for *l*th layer, i.e., '*f<sub>l</sub>*'. '*f<sub>l</sub>*' has been used to perform pooling, non-linear activation and convolution with bank of filters. As per stochastic gradient descent method, numerical optimization problem is calculated by:

$$\text{Opt}_{v_1, v_2, \dots, v_l} = \frac{1}{M} \sum_{i=1}^M \Omega(f(w^i; v_1, v_2, v_3, \dots, v_l), x^i) \quad (2)$$

where '*Ω*' denotes loss function, '*M*' is number of data.

#### 3.2.2. Rectified linear unit

Rectified linear unit (ReLU) works as an activation function. In caffe, ReLU with gradient descent is defined as (Krizhevsky et al., 2012):

$$g(r) = \max(0, r) \quad (3)$$

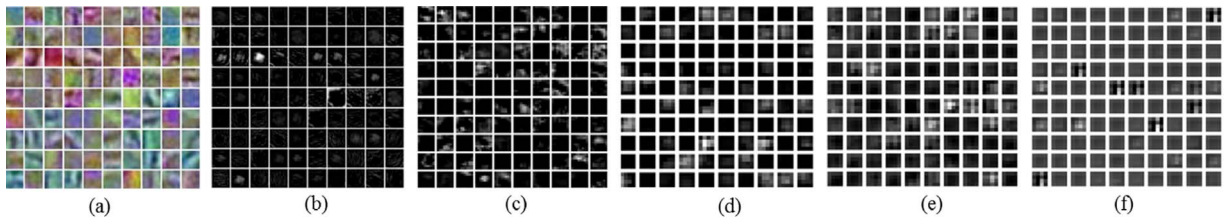


Fig. 7. Shows filters and learned features maps of the proposed deep network, (a) first layer filter (b) first hidden layer 90(10 × 9) units, (c) second hidden layer 100(10 × 10) units, (d) third hidden layer 100(10 × 10) units, (e) fourth hidden layer 100(10 × 10) units and (f) fifth hidden layer 100(10 × 10).

where, '*g*' denotes model's output function with an input '*r*'.

#### 3.2.3. Pooling layer

Pooling layer is employed to down-samples the image size by a constant factor, i.e., 2 or 3 (Masci et al., 2011). This layer improves the filter selectivity. This layer produces single output by sub-sampling the convolutional layer. We have used max-pooling layers, which consider a maximum of the block, in the model.

#### 3.2.4. Fully connected layer

In deep learning, fully connected (FC) layer works as a classifier. FC layer is not spatially located and serves as a simple vector. This layer produces an output like single vector. In the proposed model, the fully connected layer height and width of each blob are set to 1.

#### 3.2.5. Dropout layer

Dropout layer is basically used to set the hidden neurone output to zero (Krizhevsky et al., 2012). In the proposed model, dropout value is set to 0.05. The dropout neurones will not be useful for back-propagation or forward pass. This layer reduces the co-adaption complexity of neurones. In the proposed architecture, in order to avoid overfitting, the dropout layer has been included after the first fully connected layer.

#### 3.2.6. Handcrafted features layer

A lot of research articles has been dedicated to select handcrafted features in conventional mitosis detection techniques. However, it is tedious and time-consuming to mathematically describe the domain specific knowledge and human intuition. Moreover, human heuristics may not guarantee the performance of a feature on a related machine learning problem. An increasing number of papers demonstrate that handcrafted features and deep learning alone provide the best result in computer vision problem. Inspired by this concept, we compile both the techniques to achieve a better result. The handcrafted features played a vital role in the proposed architecture. We used handcrafted features issued from previous medical challenges MITOS @ ICPR 2012, AMIDA-13, and projects (MICO ANR TecSan) expertise. In our methodology, handcrafted features mainly consist of morphological, textural and intensity features (Uppuluri, 2008; Krishnan et al., 2012, 2011). The morphological features mainly signify characteristics of mitosis shape. The texture and intensity features represent textural and statistical characteristics of mitosis region. All the features have been extracted from the masked RGB image patches of training dataset. Table 3 shows the 55 Hand-crafted features extracted from the mitosis and non-mitosis image patches (\* represents significant).

### 3.3. The proposed deep learning architecture

At first, whole slide images were processed using openslide software to get HPF images. Fig. 1 shows the flow of HPF image generation (40× magnification), an image adopted from (TUPAC, 2016). Then, the HPF color images have been converted into blue ratio images (Fig. 2). The main goal of the conversion is to find the most prominent and high brightness objects within the image. Mathematically, the conversion from RGB to blue ratio image is denoted by the following equation



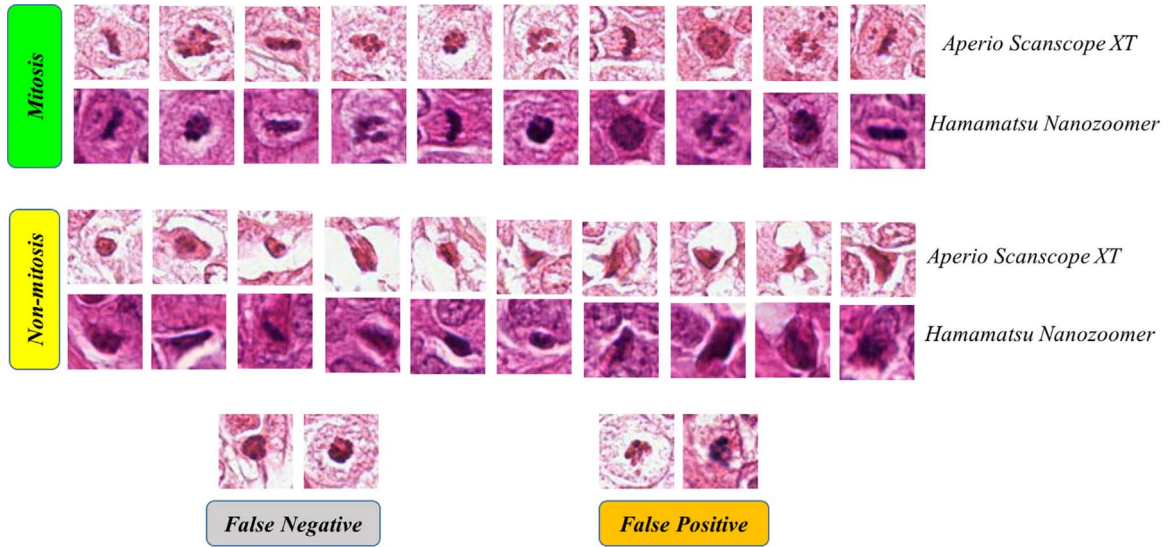


Fig. 8. The mitosis detection results.

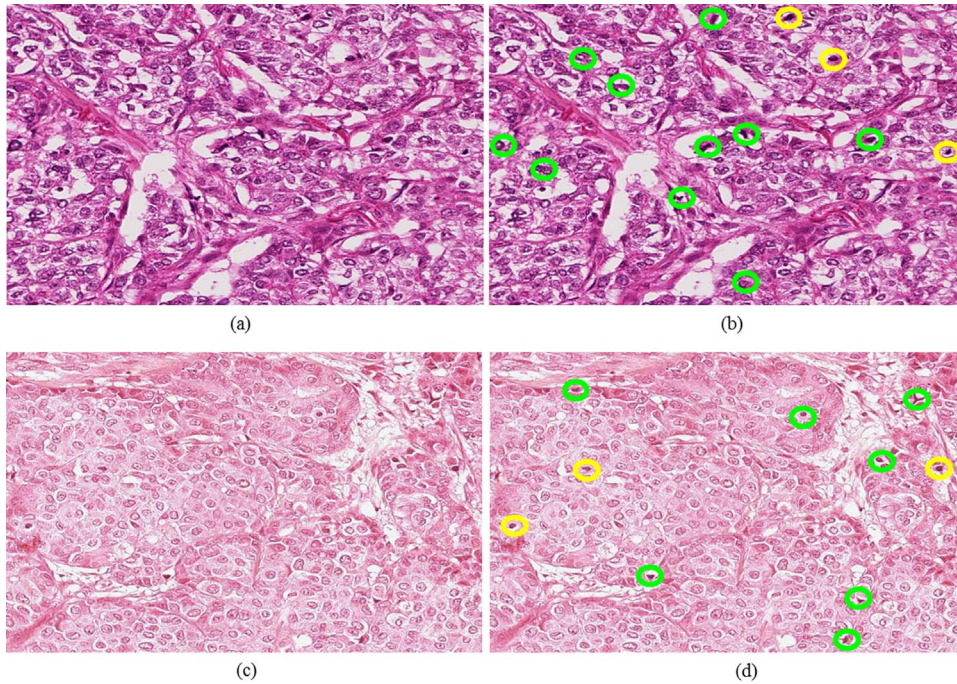


Fig. 9. The mitosis detection results on HPF images at 40× magnification, Hamamatsu scanner: (a) original image, (b) final result mitosis (yellow circle) and non-mitosis (green circle); Aperio scanner: (c) original image, (d) final result mitosis (yellow circle) and non-mitosis (green circle). (For interpretation of the references to color in this figure legend, the reader is referred to the web version of the article.)

**Table 5**  
Performance measures for mitosis detection.

Scanner types	Confusion matrix		Precision	Recall	F-score
Aperio	172	23	0.92	0.88	0.90
	13	160			
Hamamatsu	171	24	0.92	0.88	0.90
	13	160			
Average			0.92	0.88	0.90

(Chang et al., 2012):

$$\text{Blue Ratio} = \frac{100 \times B}{1 + R + G} \times \frac{256}{1 + R + G + B} \quad (4)$$

Here, 'R' denotes red channel intensity 'B' denotes blue channel intensity and 'G' denotes green channel intensity.

The blue ratio images are then processed by morphological erosion and dilation operations. The gray scale erosion is denoted by the below equation (Gonzalez et al., 2009):

$$(r \ominus s)(p, q) = \min\{r(p + p', q + q') - s(p', q') | (p', q') \in V_s\} \quad (5)$$

Here,  $(r \ominus s)$  represents binary erosion of  $r$  and the structuring element  $s$ .  $V_s$  represents the domain of the structuring element  $s$  and  $r(p, q)$  assigned to  $+\infty$ . Now, for flat structuring element, gray scale erosion will be,

$$(r \ominus s)(p, q) = \min\{r(p + p', q + q') | (p', q') \in V_s\} \quad (6)$$

where,  $s(p, q) = 0$ .

In the same way, the dilation equation for flat structuring element gray scale image is,

$$(r \oplus s)(p, q) = \max\{r(p - p', q - q') | (p', q') \in V_s\} \quad (7)$$

Erosion and dilation help in removing unnecessary objects in a blue



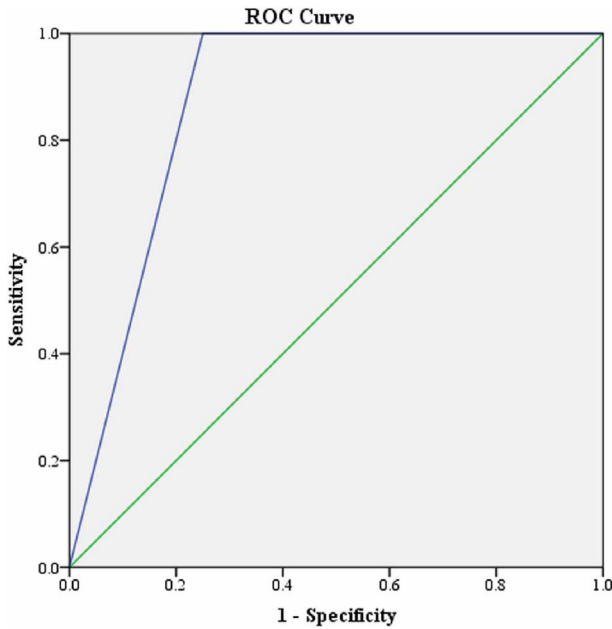


Fig. 10. ROC curve.

**Table 6**  
5-Fold cross-validation.

Cross-validation	Pr	Re	F-score
1st FOLD	0.92	0.88	0.90
2nd FOLD	0.92	0.90	0.90
3rd FOLD	0.91	0.88	0.89
4th FOLD	0.92	0.88	0.90
5th FOLD	0.92	0.87	0.89
Average	0.92	0.88	0.90

**Table 7**  
Comparison with other methodologies.

References	Pr	Re	F-score
Paul and Mukherjee (2015)	0.83	0.66	–
Wang et al. (2014a)	0.84	0.65	0.73
Cireşan et al. (2013)	0.88	0.70	0.78
Proposed method	0.92	0.88	0.90

**Table 8**  
Performance with/without handcrafted features.

Proposed method	Pr	Re	F-score
Without handcrafted features	0.86	0.69	0.76
With handcrafted features	0.92	0.88	0.90

ratio image. We found the centroid of each objects. On the basis of centroid, we crop the image into small patches (mitosis and non-mitosis). The small patches of  $w \times w = 71 \times 71 = 5041$  pixels are collected and passed to the model. To contain mitosis/non-mitosis within the above mentioned patch size under  $40\times$  magnification resolution image is enough. The non-mitosis patches do not contain any mitosis or any part of mitosis and vice-versa. For the proposed architecture, we rotated patches into  $0^\circ$ ,  $45^\circ$ ,  $90^\circ$  and  $180^\circ$  to diminish the rotation-variant issue of the input features and to increase the number of training dataset. All patches are in RGB image format. Let's, the number of color channels is denoted by  $(T) = 3$ . In the input layer of the proposed deep learning architecture, patch represents vector pixel intensity in the form of column vector. Therefore, there are  $d_x = s_0 = 3 \times 71 \times 71 = 15,123$

inputs. Here,  $2 \times 2$  region corresponds to 4 input pixels. This region is called Local receptive fields (LRF). Now, we move the LRF across the whole image. In the first input layer the LRF is being moved by one layer pixel at a time. This length is called stride length.

The proposed deep learning model has been developed using CAFFE deep learning framework (Jia et al., 2014). The model contains mainly two sections, i.e., the first section is deep architecture and the second section is handcrafted features. The deep architecture contains five convolution layer, four max-pooling layer, four ReLU, and two fully connected layer. ReLU has been used after each convolutional layer (Dahl et al., 2013). Dropout layer has been included after first fully connected layer (Srivastava et al., 2014). For better result, the dropout ratio is set to 0.05. Table 4 shows architectural details of the proposed deep framework. The workflow diagram of the proposed deep framework has been shown in Fig. 3. Fig. 4 illustrates a flow diagram of the handcrafted feature generation. The overall methodology has been described in Fig. 5. This model is inspired by Krizhevsky et al. (2012) and Deng et al. (2009). Our proposed model learns from the labeled data.

### 3.4. Parameter initialization and training

Before training, we initialize few relevant parameters (e.g., training batch size, validation batch size, the number of testing iteration, etc.). We have total 11,921 (6800 mitosis + 5,121 non-mitosis) training image patches ( $t_s$ ) and 4323 validation image patches ( $v_s$ ). Training batch size is calculated by the total number of training images processed together in a single batch. In our proposed model training batch size ( $t_{bs}$ ) is set to 256. Alternatively, validation batch size ( $v_{bs}$ ) is the total number of validation images processed together for test phase. In the proposed model, ' $v_{bs}$ ' is set to 50. Testing iteration ( $test_{itr}$ ) is calculated as:  $test_{itr} = (v_s/v_{bs})$ . Testing interval ( $test_{inv}$ ) determines how often you validate the model. Here ' $test_{inv}$ ' is set to 5000. So to cover the entire training set or completing an epoch, we have to run  $(t_s/t_{bs})$  iterations. Maximum iteration is set to 300,000, weight decay 0.005, learning rate 0.01 and momentum 0.9. The architecture was trained using stochastic gradient descent approach.

## 4. Experimental results

### 4.1. Qualitative results

Total 55 features among all categories have been extracted. After that, the Student's  $t$ -test has been performed and we got 24 significant ( $p < 0.05$ , 95% confidence interval) features out of 55 features. Fig. 6 shows the correlation matrix for 24 global features ( $p < 0.05$ ) for image classification.  $|Corrcoef(x, y)| = 1$  means highest correlation and  $|Corrcoef(x, y)| = 0$  indicates no correlation. The visualization of first layer filters and trained high-level (i.e., first, second, third, fourth and fifth hidden layer) features are shown in Fig. 7. Only 100 feature maps have been shown in each hidden layer to visualize the maps clearly. These features illustrate the proposed deep architecture, allowing the detection of mitosis from the image patches.

The qualitative and detection results of the proposed architecture have been shown in Figs. 8 and 9 respectively. In these images, the yellow circle represents the true mitosis; the green circle represents the non-mitosis. These results suggested that the proposed architecture is working well for better detection of mitosis and non-mitosis.

### 4.2. Quantitative evaluation

According to the MITOS-ATYPIA-14 challenge evaluation criteria, if the coordinates of the detected mitosis centroid to the ground truth mitosis centroid are within a range of  $8\mu m$ , then the detected mitosis will be considered as true positive (MITOS-ATYPIA, 2014). The model is quantitatively evaluated using precision ( $Pr$ ), recall ( $Re$ ) and  $F$ -score

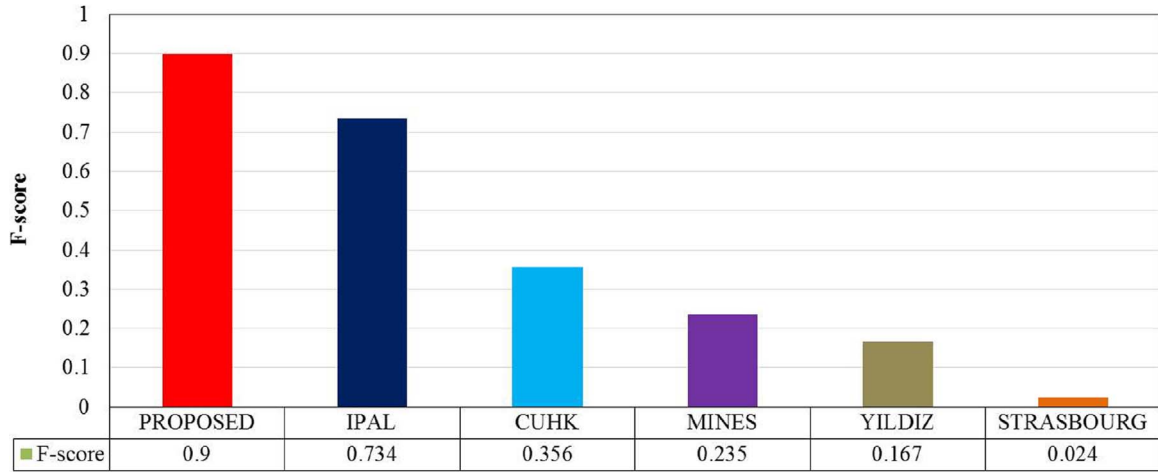


Fig. 11. Comparison of  $F$ -score values using various methods on MITOS-ATYPIA-14 dataset.

Table 9

Performance based on various combinations of training and testing dataset.

Training images (%)	Testing images (%)	$Pr$	$Re$	$F$ -score
25	75	0.92	0.88	0.90
50	50	0.93	0.88	0.90
75	25	0.94	0.89	0.91

(Xu et al., 2016).

$$F \text{ score} = 2 \times \frac{Pr \times Re}{Pr + Re} \quad (8)$$

$$Pr = \frac{\text{True Positive}}{\text{True Positive} + \text{False Positive}} \quad (9)$$

$$Re = \frac{\text{True Positive}}{\text{True Positive} + \text{False Positive}} \quad (10)$$

Table 5 shows the performance measures of Hamamatsu Nano-Zoomer 2.0-HT and Aperio Scanscope XT scanner images. The proposed model achieved 0.92 precision, 0.88 recall and 0.90  $F$ -score value. The ROC curve is shown in Fig. 10. The area under the curve is 0.875 (green line denotes the reference line). The results of Table 5 suggest that the proposed model achieves the high precision,  $F$ -score and recall value in comparison with the existing other methods. High true positive rate or precision signifies more accurate results for mitosis detection. In our problem, we only knew the total number of mitosis patches. However, we were unaware of the number of non-mitosis patches in the testing

data. Therefore, for testing the number of non-mitosis is considered for almost all non-mitosis portions in the image. The results show the importance of the model along with handcrafted feature, the relatively poor performance of the existing models or models without the handcrafted layer. It is the most interesting result of this work. Usually, people are adopting deep learning to extract features (i.e. without performing manually) automatically. In this case, the use of handcrafted ones is making things better. Table 8 shows the performance comparison table between with and without using handcrafted features. The performance measures without handcrafted features show comparatively lower precision, recall and  $F$ -score value in comparison with the proposed method. This table shows that deep learning with handcrafted features confirms mitosis and non-mitosis more accurately in comparison to the one without handcrafted features.

#### 4.3. Comparative results

We engaged 5-fold cross validation where each subset was included 20% of the total data. The each fold cross-validation performances has been shown in Table 6. Table 7 shows comparison result among most recently published articles and the proposed model. From this table, it is evident that our model performs satisfactorily regarding  $F$ -score, precision and recall value than the existing methods worked on similar kind of dataset. Fig. 11 shows the comparative graphs of  $F$ -score value on the MITOS-ATYPIA dataset. Furthermore, performances based on various combinations of training and testing dataset have been discussed in Table 9.

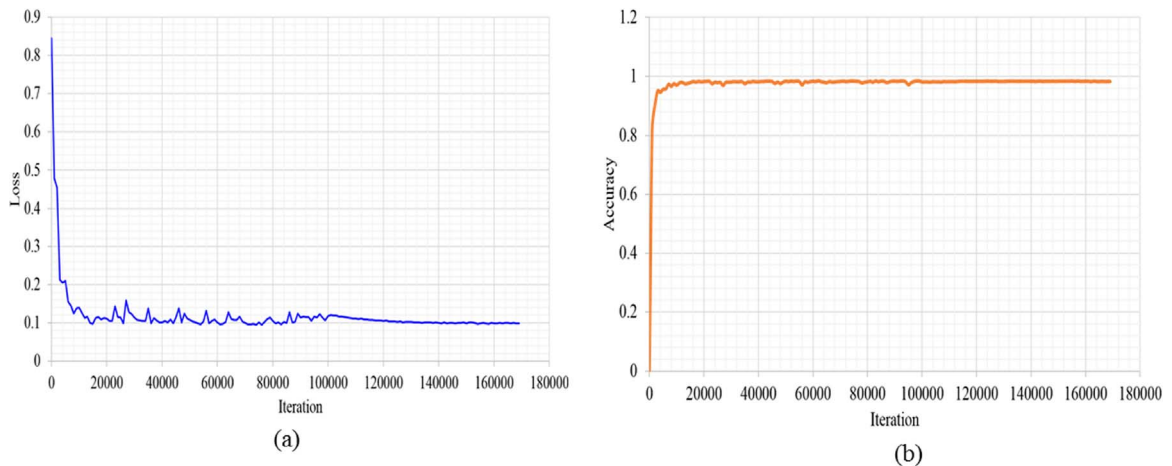


Fig. 12. Training performance graphs: (a) loss vs iteration graph and (b) accuracy versus iteration graph.

#### 4.4. Computation time

In clinical application, computation time is crucial as WSI images consist of thousands of HPFs. The superiority of our proposed model is that its detection time is very less. It took around 0.3 s for each HPF input image patch. Furthermore, the proposed cascaded framework achieved a comparable classification accuracy of 98%. It makes the framework possible for real-world clinical applications. Fig. 12 shows training performance graphs. During training, classification accuracy observed more than 98% at the 120,000 iterations.

#### 5. Discussion

Histopathological images are contaminated with subjectivity and incompleteness. These are unavoidable to morphological variation and a sheer number of mitosis. The architecture presented in this paper on the basis of dataset available in hand. An extensive network requires more training time, more variation in the representations of high-level object and expenses for other resources. In the proposed model, morphological, textural and intensity features deliver best results. Selection of input features is very much important because suitable features reduce the time duration, complexity and provide better performance.

Automatic mitosis detection from BC histopathology images could provide better benefits to pathologists in many ways. The most important application is to locate, identify and count all mitosis in HPF images. This technique could facilitate quantitative analysis, reduce intra-observer variability and remove tediousness in routine pathological practice. There has few limitation which has been discussed below:

##### 5.1. Limitations

- First, the proposed framework has been trained based on 40× magnification images. Hence, it may not work properly if lesser or higher magnification images are used.
- Second, the shape of mitotic figures is different in each of the mitosis phases which may increase false positive rate.
- Third, huge datasets are required for training using deep learning. This is one of the main obstacles the researchers may face as there are very limited standard dataset available online.
- Fourth, due to some possible variation in the slide preparation (staining process, concentration, proportion, etc.), pathologists may miss some prominent mitotic figures. These limitations can be reduced to a greater extent if the image patches are selected with proper concentration and expertise.

#### 6. Conclusion

The proposed model has been used for automated detection of mitosis in routine H&E stained BC histology images. The use of deep architecture reinforced with handcrafted features issued from three challenges increased the performance of the proposed deep learning framework. The comparison results show the strength of the proposed methodology. Moreover, the *F*-score, precision and recall value indicates better performance evaluation results as compared with the other existing techniques. The proposed deep architecture can enable classification of topological features on BC tumour histology. Finally, the presented mitosis detection model could potentially offer a useful tool to pathologists for a better understanding of BC grading.

#### Acknowledgements

We would like to acknowledge Department of Science and Technology (DST), Govt. of India, for providing the INSPIRE fellowship (IVR Number: 201400105113) and Indo-French Centre for Promotion of Advanced Research (CEFIPRA) for Raman-Charpak fellowship 2015

(RCF-IN-0071). C. Chakraborty acknowledges Ministry of Human Resource Development (MHRD), Govt. of India for partial support to carry out this work (grant no: 4-23/2014 T.S.I. date: 14-02-2014).

The major part of this research work has been carried out at Laboratoire d'Imagerie Biomédicale (LIB), University Pierre and Marie Curie (UPMC-Paris 6), Paris, France under the guidance of Prof. Daniel Racocanu. The authors are thankful to Philippe DUMÉE, LIB, (UPMC-Paris 6) for his helpful support to carry out this research.

#### References

- Albarqouni, S., Baur, C., Achilles, F., Belagiannis, V., Demirci, S., Navab, N., 2016. Aggnet: deep learning from crowds for mitosis detection in breast cancer histology images. *IEEE Trans. Med. Imaging* 35 (5), 1313–1321.
- Assessment of Mitosis Detection Algorithms 2013 (AMIDA13), 2016. <http://amida13.isi.uu.nl/> (accessed 24.10.16).
- Aptoula, E., Courty, N., Lefèvre, S., 2013. Mitosis detection in breast cancer histological images with mathematical morphology. In: *Signal Processing and Communications Applications Conference (SIU)*, 2013 21st. IEEE. pp. 1–4.
- Chang, H., Loss, L.A., Parvin, B., 2012. Nuclear segmentation in H&E Sections via multi-reference graph cut (MRGC). *International Symposium Biomedical Imaging*.
- Cireşan, D.C., Giusti, A., Gambardella, L.M., Schmidhuber, J., 2013. Mitosis detection in breast cancer histology images with deep neural networks. In: *International Conference on Medical Image Computing and Computer-Assisted Intervention*. Springer. pp. 411–418.
- Dahl, G.E., Sainath, T.N., Hinton, G.E., 2013. Improving deep neural networks for LVCSR using rectified linear units and dropout. In: *2013 IEEE International Conference on Acoustics, Speech and Signal Processing*. IEEE. pp. 8609–8613.
- Deng, J., Dong, W., Socher, R., Li, L.-J., Li, K., Fei-Fei, L., 2009. Imagenet: a large-scale hierarchical image database. In: *IEEE Conference on Computer Vision and Pattern Recognition*, 2009. CVPR 2009. IEEE. pp. 248–255.
- Elston, C.W., Ellis, I.O., 1991. Pathological prognostic factors in breast cancer. I. The value of histological grade in breast cancer: experience from a large study with long-term follow-up. *Histopathology* 19 (5), 403–410.
- Giusti, A., Caccia, C., Cireşari, D.C., Schmidhuber, J., Gambardella, L.M., 2014. A comparison of algorithms and humans for mitosis detection. In: *2014 IEEE 11th International Symposium on Biomedical Imaging (ISBI)*. IEEE. pp. 1360–1363.
- Gonzalez, R.C., Woods, R., Eddins, S., 2009. Vol. 2. *Digital Image Processing Using Matlab*.
- Huang, C.-H., Lee, H.-K., 2012. Automated mitosis detection based on exclusive independent component analysis. In: *2012 21st International Conference on Pattern Recognition (ICPR)*. IEEE. pp. 1856–1859.
- Huh, S., Bise, R., Chen, M., Kanade, T., et al., 2011. Automated mitosis detection of stem cell populations in phase-contrast microscopy images. *IEEE Trans. Med. Imaging* 30 (3), 586–596.
- International Conference on Pattern Recognition (ICPR) – 2012, 2012. [http://ludo17.free.fr/mitos\\_2012/dataset.html](http://ludo17.free.fr/mitos_2012/dataset.html) (accessed 03.10.16).
- Irshad, H., et al., 2013a. Automated mitosis detection in histopathology using morphological and multi-channel statistics features. *J. Pathol. Inform.* 4 (1), 10.
- Irshad, H., Jalali, S., Roux, L., Racocanu, D., Hwee, L.J., Le Naour, G., Capron, F., et al., 2013b. Automated mitosis detection using texture, sift features and hmax biologically inspired approach. *J. Pathol. Inform.* 4 (2), 12.
- Irshad, H., Gouaillard, A., Roux, L., Racocanu, D., 2014a. Multispectral band selection and spatial characterization: application to mitosis detection in breast cancer histopathology. *Comput. Med. Imaging Graph.* 38 (5), 390–402.
- Irshad, H., Gouaillard, A., Roux, L., Racocanu, D., 2014b. Spectral band selection for mitosis detection in histopathology. In: *2014 IEEE 11th International Symposium on Biomedical Imaging (ISBI)*. IEEE. pp. 1279–1282.
- Traore, L., Daniel, C., Jaulent, M.-C., Schrader, T., Racocanu, D., Kergosien, Y., 2016. A sustainable visual representation of available histopathological digital knowledge for breast cancer grading. *Diagn. Pathol. J.* 2 (1).
- Jia, Y., Shelhamer, E., Donahue, J., Karayev, S., Long, J., Girshick, R., Guadarrama, S., Darrell, T., 2014. Caffe: convolutional architecture for fast feature embedding. In: *Proceedings of the 22nd ACM International Conference on Multimedia*. ACM. pp. 675–678.
- Kayser, K., Borkenfeld, S., Carvalho, R., Djenouni, A., Kayser, G., 2016. How to analyze structure and function in tissue-based diagnosis? *Diagn. Pathol.* 2 (1).
- King, R.J.B., Robins, M.W., 2006. *Cancer Biology*. Pearson Education.
- Krishnan, M.M.R., Choudhary, A., Chakraborty, C., Ray, A.K., Paul, R.R., 2011. Texture based segmentation of epithelial layer from oral histological images. *Micron* 42 (6), 632–641.
- Krishnan, M.M.R., Pal, M., Paul, R.R., Chakraborty, C., Chatterjee, J., Ray, A.K., 2012. Computer vision approach to morphometric feature analysis of basal cell nuclei for evaluating malignant potentiality of oral submucous fibrosis. *J. Med. Syst.* 36 (3), 1745–1756.
- Krizhevsky, A., Sutskever, I., Hinton, G.E., 2012. Imagenet classification with deep convolutional neural networks. *Advances in Neural Information Processing Systems*. pp. 1097–1105.
- Liu, A., Li, K., Kanade, T., 2010. Mitosis sequence detection using hidden conditional random fields. In: *2010 IEEE International Symposium on Biomedical Imaging: From Nano to Macro*. IEEE. pp. 580–583.
- Lo, S.-C.B., Chan, H.-P., Lin, J.-S., Li, H., Freedman, M.T., Mun, S.K., 1995. Artificial



- convolution neural network for medical image pattern recognition. *Neural Netw.* 8 (7), 1201–1214.
- Malon, C., Brachtel, E., Cosatto, E., Graf, H.P., Kurata, A., Kuroda, M., Meyer, J.S., Saito, A., Wu, S., Yagi, Y., 2012. Mitotic figure recognition: agreement among pathologists and computerized detector. *Anal. Cell. Pathol.* 35 (2), 97–100.
- Malon, C.D., Cosatto, E., et al., 2013. Classification of mitotic figures with convolutional neural networks and seeded blob features. *J. Pathol. Inform.* 4 (1), 9.
- Masci, J., Meier, U., Cireşan, D., Schmidhuber, J., 2011. Stacked convolutional auto-encoders for hierarchical feature extraction. In: *International Conference on Artificial Neural Networks*. Springer, pp. 52–59.
- Mazia, D., 1961. Mitosis and the physiology of cell division. *Cell* 3, 77–412.
- MITOS-ATYPIA 14, 2014. <https://grand-challenge.org/site/mitos-atypia-14/home/> (accessed 24.10.16).
- Nateghi, R., Danyali, H., Sadegh-Helfroush, M., Pour, F.P., 2014. Automatic detection of mitosis cell in breast cancer histopathology images using genetic algorithm. In: *2014 21st Iranian Conference on Biomedical Engineering (ICBME)*. IEEE, pp. 1–6.
- O'Brien, C.A., Pollett, A., Gallinger, S., Dick, J.E., 2007. A human colon cancer cell capable of initiating tumour growth in immunodeficient mice. *Nature* 445 (7123), 106–110.
- Paul, A., Mukherjee, D.P., 2015. Mitosis detection for invasive breast cancer grading in histopathological images. *IEEE Trans. Image Process.* 24 (11), 4041–4054.
- Rakha, E.A., Reis-Filho, J.S., Baehner, F., Dabbs, D.J., Decker, T., Eusebi, V., Fox, S.B., Ichi-hara, S., Jacquemier, J., Lakhani, S.R., et al., 2010. Breast cancer prognostic classification in the molecular era: the role of histological grade. *Breast Cancer Res.* 12 (4), 1.
- Roullier, V., Lézoray, O., Ta, V.-T., Elmoataz, A., 2011. Multi-resolution graph-based analysis of histopathological whole slide images: application to mitotic cell extraction and visualization. *Comput. Med. Imaging Graph.* 35 (7), 603–615.
- Roux, L., Racocceanu, D., Loménie, N., Kulikova, M., Irshad, H., Klossa, J., Capron, F., Genestie, C., Naour, G., Gurcan, M., 2013. Mitosis detection in breast cancer histological images an icpr 2012 contest. *J. Pathol. Inform.* 4 (1), 8. <http://dx.doi.org/10.4103/2153-3539.112693>.
- Saha, M., Agarwal, S., Arun, I., Ahmed, R., Chatterjee, S., Mitra, P., Chakraborty, C., 2015. Histogram based thresholding for automated nucleus segmentation using breast imprint cytology. *Advancements of Medical Electronics*. Springer, pp. 49–57.
- Saha, M., Mukherjee, R., Chakraborty, C., 2016a. Computer-aided diagnosis of breast cancer using cytological images: a systematic review. *Tissue Cell* 48 (5), 461–474.
- Saha, M., Arun, I., Basak, B., Agarwal, S., Ahmed, R., Chatterjee, S., Bhargava, R., Chakraborty, C., 2016b. Quantitative microscopic evaluation of mucin areas and its percentage in mucinous carcinoma of the breast using tissue histological images. *Tissue Cell* 48 (3), 265–273.
- Saha, M., Chakraborty, C., Arun, I., Ahmed, R., Chatterjee, S., 2017. An advanced deep learning approach for Ki-67 stained hotspot detection and proliferation rate scoring for prognostic evaluation of breast cancer. *Sci. Rep.* 7 (1), 3213.
- Schlachter, M., Reisert, M., Herz, C., Schlurmann, F., Lassmann, S., Werner, M., Burkhardt, H., Ronneberger, O., 2010. Harmonic filters for 3d multichannel data: rotation invariant detection of mitoses in colorectal cancer. *IEEE Trans. Med. Imaging* 29 (8), 1485–1495.
- Sharma, H., Zerbe, N., Lohmann, S., Kayser, K., Hellwich, O., Hufnagel, P., 2015. A review of graph-based methods for image analysis in digital histopathology. *Diagn. Pathol.* 1 (1).
- Sirinukunwattana, K., Raza, S.E.A., Tsang, Y.-W., Snead, D.R., Cree, I.A., Rajpoot, N.M., 2016. Locality sensitive deep learning for detection and classification of nuclei in routine colon cancer histology images. *IEEE Trans. Med. Imaging* 35 (5), 1196–1206.
- Srivastava, N., Hinton, G.E., Krizhevsky, A., Sutskever, I., Salakhutdinov, R., 2014. Dropout: a simple way to prevent neural networks from overfitting. *J. Mach. Learn. Res.* 15 (1), 1929–1958.
- Tao, C.Y., Hoyt, J., Feng, Y., 2007. A support vector machine classifier for recognizing mitotic subphases using high-content screening data. *J. Biomol. Screen.* 12 (4), 490–496.
- Tashk, A., Helfroush, M.S., Danyali, H., Akbarzadeh, M., 2013. An automatic mitosis detection method for breast cancer histopathology slide images based on objective and pixel-wise textural features classification. In: *2013 5th Conference on Information and Knowledge Technology (IKT)*. IEEE, pp. 406–410.
- Tashk, A., Helfroush, M., Danyali, H., Akbarzadeh, M., 2014. A novel cad system for mitosis detection using histopathology slide images. *J. Med. Signals Sens.* 4 (2), 139–149.
- Tek, F.B., et al., 2013. Mitosis detection using generic features and an ensemble of cascade adaboosts. *J. Pathol. Inform.* 4 (1), 12.
- Tripathi, A.S., Mathur, A., Daga, M., Kuse, M., Au, O.C., 2013. 2-SiMDoM: a 2-sieve model for detection of mitosis in multispectral breast cancer imagery. In: *2013 IEEE International Conference on Image Processing*. IEEE, pp. 611–615.
- Tumor Proliferation Assessment Challenge 2016 (TUPAC16), 2016. <http://tupac.tue-image.nl/> (accessed 24.10.16).
- Uppuluri, A., 2008. GLCM Texture Features. <https://in.mathworks.com/matlabcentral/fileexchange/22187-glcmm-texture-features>.
- Üstüner, M., Bilgin, G., 2015. Mitosis detection on histopathological images using statistical detection algorithms. In: *2015 23rd Signal Processing and Communications Applications Conference (SIU)*. IEEE, pp. 540–543.
- Veta, M., Van Diest, P.J., Willems, S.M., Wang, H., Madabhushi, A., Cruz-Roa, A., Gonzalez, F., Larsen, A.B., Vestergaard, J.S., Dahl, A.B., et al., 2015. Assessment of algorithms for mitosis detection in breast cancer histopathology images. *Med. Image Anal.* 20 (1), 237–248.
- Veta, M., van Diest, P.J., Jiwa, M., Al-Janabi, S., Pluim, J.P., 2016. Mitosis counting in breast cancer: object-level interobserver agreement and comparison to an automatic method. *PLOS ONE* 11 (8), e0161286.
- Wang, H., Cruz-Roa, A., Basavanahally, A., Gilmore, H., Shih, N., Feldman, M., Tomaszewski, J., Gonzalez, F., Madabhushi, A., 2014a. Cascaded ensemble of convolutional neural networks and handcrafted features for mitosis detection. In: *SPIE Medical Imaging*. International Society for Optics and Photonics, pp. 90410B.
- Wang, H., CruzRoa, A., Basavanahally, A., Gilmore, H., Shih, N., Feldman, M., Tomaszewski, J., Gonzalez, F., Madabhushi, A., 2014b. Mitosis detection in breast cancer pathology images by combining handcrafted and convolutional neural network features. *J. Med. Imaging (Bellingham, Wash.)* 1 (3) 034003-034003.
- Xu, J., Xiang, L., Liu, Q., Gilmore, H., Wu, J., Tang, J., Madabhushi, A., 2016. Stacked sparse autoencoder (SSAE) for nuclei detection on breast cancer histopathology images. *IEEE Trans. Med. Imaging* 35 (1), 119–130.